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SYSTEM AND PROCESS DEVELOPMENT FOR SELECTION OF HIGH STRESS TOLERANCE PERSONNEL

by Albert F. Ax

NASA CR-1122

Prepared by LAFAYET'TE CLINIC Detroit, Mich. for Ames Research Center

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Prepared under Contract No. NAS 2-1031 by LAFAYETTE CLINIC Detroit Mich.

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NATIONAL AERONAUTICS AND SPACE ADMINISTRATION

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ABSTRACT

A system has been developed for digital computer processing of psychophysiological data. It employs oscilloscope and oscillograph display, analog magnetic tape storage, A/D conversion, digital tape storage and a large digital computer (IBM 7094). The computing programs developed select all points of interest and compute their type, time of occurence, amplitude and curvature. A summary program computes the mean and standard deviation for the response parameters of amplitude, slope, curvature, duration and interval for any set of epochs selected by the editor. A third program selects pairs of points from any sets of variables on the basis of minimizing the variance in lag for the set. The coincidence coefficient and product moment correlations are computed for any set of response parameters of paired points chosen by the editor. These correlations do not confound coincidence, amplitude and shape of responses as does the classical cross-correlation function and are therefore more suitable for the study of the interdependence of biological subsystems.

Two substantive studies have been completed. The classical conditioning of autonomic responses in schizophrenia and healthy subjects demonstrated a marked impairment in the performance of autonomic conditioning by schizophrenic patients. A pilot study of non-schizophrenic low motivation subjects revealed a disability for autonomic conditioning similar to that found in chronic schizophrenia. These findings suggest that autonomic conditioning may serve as an index for the diagnosis of both schizophrenia and low motivation and permit the speculation that a low aptitude for autonomic learning may be a contributing factor to both schizophrenia and low social motivation. Finally a study of physiological concomitants of psychological differentiation suggests that the

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degree of autonomic response differentiation may be correlated with the cognitive style of perceptual discrimination.

It was concluded that these successful demonstrations of the diagnostic power of psychophysiological data and those of digital computer analysis justify further study and development of this approach.

These studies are of value to NASA and the science of human motivation and emotional development by virtue of progressing toward more accurate selection and rapid training of personnel for high stress tasks.

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I. Purposes of the Study.

The primary purposes of this study were to develop a system for processing psychophysiological data and to apply it to the task of developing indices for the diagnosis of human tolerance for stress. It was recognized that aptitudes for learning motives and emotional control were primary components of stress tolerance. In order to contain the scope of the investigation within practicable limits imposed by our resources only the psychophysiological aspects of motivation and learning were considered.

The context of the study has two salient features. The psychophysiology laboratory at The Lafayette Clinic had just completed the development of a processing system for psychophysiological data utilizing and EPSCO data logger consisting of a 29 channel multiplexor and a 10 Kc A/D converter and a Bendix G15-D computer with special programs developed for the purpose. That study demonstrated the approach to be feasible but relatively impracticable because of the limitations in capacity and speed of the computer. The other favorable aspect of the situation was that the state-of-the-art of the psychophysiological methodology was just approaching the level to justify major effort toward massive data processing. Biomedical monitoring was being used with pilots, astronauts and in hospitals. Active research was under way in several score laboratories supported by federal agencies, private industry and at medical schools and hospitals. The Society for Psychophysiological Research had been organized two years previously (1960) and the journal PSYCHOPHYSIOLOGY was being established. Psychophysiology thus appeared to be mature enough for marriage to a high speed data processing system.

Psychophysiology is one of the approaches which seeks to explain the physiology of behavior. It focuses on covert behavior available for measurement at the skin surface. It utilizes electrodes and sensitive transducers to sense physiological processes in target organs of the autonomic and central nervous systems and of the endocrine systems. Its special advantages are: (1) that its methods can obtain quantitative, continuous measurements of vital processes whose changes are often too small or fleeting to observe clinically: (2) the measurements can be made without seriously disturbing the processes being observed by intrusions such as implanted electrodes; and (3) the data obtained are already organized in terms of the target organs.

Psychophysiology has its special problems to overcome. (1) Each target organ response may be an end product of several influences, hence may not be a pure measure of any one. (2) This complexity of determination requires the simultaneous measurement of several variables so as to "triangulate" on the processes of interest. (3) The multiple variable approach necessitates complex recording and data processing equipment.

The study of intact systems without subsystem isolation (often referred to as "closed loop analysis") is sometimes criticized as unproductive for the study of the human organism because the system is so large and complex, the transfer functions so poorly described and the number of available variables so small relative to the complexity of the system that the correct interpretation of findings may be impossible. In a sense the description and prediction of human behavior is like describing and predicting the weather--both are large, complex, open, dynamic systems requiring multiple variable, closed loop analysis. More accurate prediction for both require more variables, more observation points and more sophisticated data processing than has so far been possible.

During the past 20 years large scale computers have been applied to weather prediction enabling marked advances in accuracy. We believe similar progress can be made for limited areas of human behavior such as stress tolerance, motivation and emotional control.

The analogy between weather and behavior should not be pushed too far. There are many obvious differences. One important difference is that weather is determined largely by energy transfer whereas behavior is controlled chiefly by the transfer of information. Hence the principles of information theory rather than energy transfer functions are more appropriate for the study of behavior of living organisms. Signal recognition and signal production with multiple level feedback interactions are characteristic of living organisms. For this reason the experimental design and the data processing must be appropriate to signal manipulation which involve sensory thresholds, adaptation or learning, reinforcement or motivation, differentiation and generalization. We have discussed this psychophysiological position in more detail elsewhere (Ax, 1964). An appreciation of this viewpoint is helpful for the reader to understand certain features of the experimental design, the data processing, hardware and the computer programs, as well as our interpretation of the results.

One limitation which psychophysiology shares with all science (except possibly astronomy) is the "general principle of uncertainty" used in the sense that our observations influence the phenomena under observation. The attempt to measure simultaneously as many variables as possible, to control the local environment and to standardize all procedures and instructions to subjects, etc. may influence the subject's behavior, especially his natural emotions, to such

an extent that every effort to increase these laudable scientific controls is defeated by a "law of diminishing return". Good psychophysiologic technique strives to minimize the influence of the observation procedures by employing miniature non-painful sensors and by creating a test situation as natural as The use of telemetry to replace the umbilical linkage is one possible. further step that is being taken to enable psychophysiological observation on the free roaming individual while pursuing his natural activities. This next step in psychophysiological methodology adds a severe burden to the data processing. Much more noise is introduced due to movement artifacts and uncontrolled environmental influences as well as the degradation of the signal by the radio linkage. The problems of noise elimination and pattern recognition problems for machine editing has been discussed previously (Ax, Andreski, Courter, DiGiovanni, Herman, Lucas, and Orrick, 1964) and later in this report. Recording may be carried out over days or weeks which strains both the sensor reliability and the capacity of the data processing system. Sampling rates and programming must be carefully planned to minimize the computing time and cost while at the same time maximizing information obtained. Only just sufficient redundancy of sampling to achieve reliability can be tolerated.

One final general aspect of the psychophysiological approach should be mentioned before plunging into the details of the study. Psychophysiology has certain characteristics, advantages and disadvantages as compared to the classical physiological methods. The chief advantage is its ability to obtain information about physiological system status and process without damage or discomfort to the organism. A second advantage is the organization of the response system provided by the end organs. The vasoconstriction response at a finger tip is often much easier to interpret as a functional response relevant

to the organismic intentions than is the neuronal response train from an electrode implanted deep in the brain. Similarly, the current activities of the brain may more readily and understandably be described by a pattern of end organ responses such as arterial tonus, muscle tonus, heart rate, heart stroke force, blood pressures and palmar sweating than it can from the EEGs from 32 electrodes scattered about on the scalp. The "face validity" of the EEG as a prime psychophysiological measure for brain activity has often been overvalued due to its success in helping to locate a gross physical damage of the brain. Actually the neurological examination (a clinical type of psychophysiological examination) is often more definitive for brain malfunction. Many psychophysiological variables other than EEG are excellent indices of arousal or motivational state. EEG is one useful physiological measure but has little special value simply because its sensors are located physically closest to brain tissue. A. T.V. repairman does not diagnose a malfunction by scanning the electric field strength over the cabinet of the T.V.; rather he measures potentials and currents in logically critical circuit points. The sensor and effector organs of the body are logical points for the organism. No criticism is implied of the excellent studies of brain structure and functions by direct examination of brain tissue by neurophysiologial methods. It is emphasized that total organismic processes such as emotion, motivation and "stress tolerance" are much more likely to be monitorable by patterns of end organ responses than by scalp EEG.

II. METHODS

A. Data Acquisition System.

Research employing continuous recording of multiple variables requires high speed computing for two reasons: (1) to transcribe the necessarily large numbers of samples into digital values and (2) to compute the multiple interactions among the variables involved. The transcription aspect for a single one hour session for only 10 physiological variables (not including EEG) may require as many as 36,000 samples to describe the variables. An average study of 5 sessions per subject and 100 subjects would produce 18,000,000 values; and many studies might require more variables, more recording per subject, or faster changing variables (such as EEG) which would greatly increase the amount of data to be transcribed and summarized. The computing aspect merely for means, variances, t-tests, and correlations among the parameters that can be abstracted from a set of 10 physiological variables is quite a large task without the aid of a digital computer. When more sophisticated statistics such as factor analysis and multiple regression are employed the computing multiplies many fold. Any method of processing such data less powerful than the digital computer is impracticable for large scale studies required for exploitation of the psychosychophysiologic approach.

A brief preview of some of the problems encountered in developing a high speed system for processing psychophysiologic data may be of interest. Analog computing was considered and rejected as impracticable because an analog computer sufficiently large to handle all variables simultaneously in real time would be too costly. Analysis of single variables or pairs for correlation

from magnetic tape storage by a medium-sized analog computer would probably be practicable but still probably slower and require a more costly installation although this approach might have been competitive to the digital system. A further reason for going digital is that automatic computing by the stored program digital computer is very efficient and flexible.

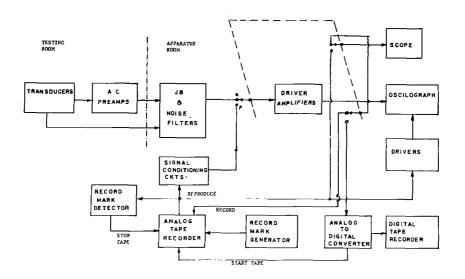
Once the specific digital computer to be used had been identified (for us an IBM 7094), then all design characteristics had to be made compatible with it. The digital tape recorder must meet 7094 specs; the AD converter must produce the specified format, packing density, parity bit, and other specifications. The ADC must have sufficient resolution which for us was 12 bits (1 part in 4096) to cover any range expected. For example if the palmar skin resistance has a range from 30,000 to 1,000,000 ohms and if a GSR as small as 200 ohms change is to be resolved the full dynamic range of 12 bits is needed. The multiplexor must be able to sample at a rate sufficient to sample all variables sufficiently fast to resolve the most rapid changes to be encountered. We judged that 10 samples per minimum expected period would be adequate. For a selection of 30 variables of varying rates of change we chose 160 samples per second real time for all 30 variables (10 at 10 per second, 10 at 5 per second and 10 at 1 per second). A multiplexor with 30 inputs was chosen with an eye to expansion but experience has shown that other difficulties and limitations make it unlikely that more than 10 to 15 variables can be handled, unless groups of subjects are studied simultaneously.

On-line analog preprocessing of most variables in various degrees is required. Nearly all variables require some filtering. Some variables like EKG for our purposes of obtaining heart rate require a cardiotachometer to detect the time of the QRS complex and convert the time between adjacent

QRS complexes into a voltage to be presented to the ADC. The step change, square wave aspect of cardiotachometer data makes it difficult to use. Most sample-and-hold circuits drift slightly and in opposite directions depending on whether the value is above or below zero potential; thus the high or low point to be picked by the computer might be either at the beginning or end of the heart cycle and thus make ambiguous the time of the point. The solution to this problem appears to be to produce a pulse at the time of the QRS whose amplitude represents the duration of the last HP and whose duration is greater than one ADC sample period but less than two, thus assuring a sample as early as possible after the information is available but none at any other time. Between readings the cardiotachometer would assume a value off scale enabling the computer to readily ignore those valueless samples.

Other problems that must be handled for automatic data processing involve solutions to the noise or artifact problem and precise calibration through the entire system from transducer to computer. Filtering and human editing (described in detail in the software section) take care of the artifact problem. Automatic editing seen as a problem of computer pattern recognition is considered a research and development problem. Practicable total system calibration requires excellent stability of component systems both as to gain and base line. A practicable system must be able to be quickly checked and adjusted by the operator and not require an engineer. Finally short term instability should be self checking possibly by supplying frequent calibration signals to the computer which could then modify the output conversion values so as to make them correct.

1. Overview.



The block diagram of Figure 1 shows the plan of the system.

Figure 1

The sensors on the subject and the preamplifiers are in the observation room. The rest of the apparatus is in the adjacent instrument room. During a recording session, the amplified signals are displayed on an 8-channel oscilloscope and recorded on a 24-channel oscillograph and on a 14-channel FM magnetic tape recorder. For computer analysis at a later time, the signals are reproduced from the tape recorder, modified by signal conditioning circuitry, rerecorded on the oscillograph, sampled and digitized by the 29-channel analog-to-digital converter (ADC) and recorded on a digital magnetic tape in IBM 7094 format.

2. Observation Situation.

The subject room is 12x14x8 feet, accoustically insulated and

temperature controlled to 25.5 ± 0.2 C. Humidity is uncontrolled but is recorded as are the outside environmental conditions of temperature, humidity, and barometric pressure. Two one-way observation ports and complete intercom with audio magnetic tape recording are provided. The subject enters directly from a corridor (not through apparatus room) and reclines on the ballistocardiograph bed. Sensors are applied and plugged into jack panels on either side at the head of the bed. Preamplifiers are near the subject for EMG, EEG, EKG, finger pulse and body movement.

3. Sensors.

(a) Electrodes.

Variables sensed by electrodes are the electrocardiogram (EKG), electroencephalogram (EEG), electromyogram (EMG), impedance plethysmogram (IPG), skin potential (SP), and skin conductance (SC). Other electrodes are used for grounding the subject and for applying electrical stimulation.

(b) Transducers.

These are used for sensing skin temperatures (ST), chest and abdominal circumference to measure respiration (CR & AR), the ballistocardiogram (BCG), finger pulse (FP), body movements (BM), and blood pressures (SBP, DBP).

4. Display and Recording.

All signals, except muscle potentials, after preamplification associated with their transducers are filtered and amplified by Offner type 492 DC amplifiers. The signal is then split into three: one branch goes to the 17", 8-channel oscilloscope and is recorded on an oscillograph (24-channel, model 1108 Honeywell) and the third branch goes to the analog magnetic tape recorder (Ampex model CP 100, 14-channel FM). Several signals may be multipexed on the oscilloscope and tape recorder so as to accommodate them all.

During the recording phase, a 1-per-second timing pulse (of 300 CPS for a period of 50 MS) is recorded on the face temperature channel. An electronic counter causes every tenth signal to actuate a marker channel of the oscillo-graph.

5. Identification Mark for Analog Tape.

Since several experimental sessions may be recorded on one roll of magnetic tape, a system is required for marking and locating the beginning of specified records. This record start mark is recorded on the tape and also displayed on the oscillograph chart, so that precise synchronization can be achieved between the record made during recording and the one made during reproduce which is used for editing. The record mark is a decimal number coded in binary by two voltage levels on each of the 14 channels of the analog tape. Its maximum value is 3999. Each recording session is given a sequential identification number (ID). A particular record may be located on a reel of analog magnetic tape by setting the decimal controls at the desired ID number. The ID numbers are displayed on Nixie tubes as they are passed and the tape stops on the preset ID number. By adding an additional unit any point within a record could be located to the nearest second. We have not found any need for this feature, hence, it has not been added, in line with our general philosophy of keeping the apparatus as simple as possible consistent with required performance.

B. Data Processing System.

1. Signal Conditioning.

Since the ADC sampling switch requires either a synchronized signal or the continuous presence of the signal, the discontinuous asynchronous pulse variables such as EKG, plethysmogram and BCG require transformation before conversion. The EKG is used to generate the heart period (HP), the peripheral

pulse amplitude of the finger plethysmogram (FP) is detected by a peak reading hold circuit, and for BCG the IJ wave is measured and held until the next EKG opens the gate for the next BCG signal. The EMG and body movements are integrated, sampled and held. EEG may be analyzed directly in the high-speed mode or it may be divided into several frequency bands and each band displayed as a continuous voltage equivalent to the smoothed average power or voltage of the signal within the band. Any period of EEG record can be analyzed in the high-speed mode of the regular "Points of Interest" program described in the section on software. Since, however, this type of micro-analysis can be quite costly, the more economical, though less detailed method of abstracting the average voltage or power from several broad bands is more practicable.

The DC or slowly changing variables such as temperatures, respiration, palmar conductance and skin potential are reproduced from the analog tape and sent to the ADC essentially unchanged except for amplification and filtering.

The signal conditioning circuitry is the stage where automatic editing for artifacts will be done. At present only filtering, gating by EKG for BCG and PP and the simple pattern recognition of the IJ portion of the BCG are used. More sophisticated pattern recognition circuits are being designed to better distinguish between clean signals and artifacts. Most artifacts caused by subject movements are now removed by the human editor as described in b, (4) of the software section.

2. Digital Magnetic Tape Formats and Sampling Rates.

Economy in digital computation requires the minimum sampling rates consistent with the type of information desired for each variable. It was decided that a sampling rate of 10 samples per minimum interval of variable would provide sufficiently detailed information for our purposes.

Thus if maximum respiration rate were 1 per second, 10 samples per second would enable sufficiently accurate location and amplitude determinations required for computing respiration period and an index of tidal volume. Similary the heart period can change from a maximum of about 2.0 seconds to a minimum of about .33 seconds (30 to 180 beats per minute) in not less than 1/3 second. A sampling rate of 3 SPS would suffice; but because of our desire to correlate the coincidence of changes as well as amplitude changes of heart and respiration periodicity, it was decided to sample the cardiac variables also at 10 SPS so as to make the time of corresponding points on correlated variables equally precise. The slow-changing variables like temperature and those integrated for a definite time of 1 second are sampled 1 SPS. A sampling rate of 5 SPS was chosen for skin potential. In order to provide for the future addition of variables, the ADC sampling switch was designed to provide 10 variables at 10 SPS, 10 at 5 SPS and 10 at 1 SPS including a nonsampled time code generated at 1 SPS. Together these total 160 SPS in real time or 1280 SPS in the reproduce mode as actually used (8:1 speedup). Because of the inherent high-speed sampling and conversion capability of the solid state converter, and an expectation that higher frequency variables such as EEG might sometime be analyzed, a high-speed mode of 6400 SPS is also available. Thus for the high-speed mode there are 10 channels each at 400 SPS, 10 at 200 SPS and 10 at 40 SPS. When this mode is used, the analog record and playback is 1:1 and the digital tape operates at 25"/sec producing the same bit density of 512/inch used for the low-speed mode in which the tape speed is 5"/sec.

a. Density and Sampling Rate.

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The raw data is recorded on a digital tape for input

to a 7094. The tape is recorded at 512 bits/inch in binary (odd parity) mode. The data is recorded in long physical records with the data samples packed and interlaced. The present system accommodates 30 channels of data sampled at 3 different frequencies.

Channe1s	1 - 10	Sampled 1) times/second.
Channels	11 - 20	Sampled	5 times/second.
Channels	21 - 30	Sampled	l time/second.

Channel 30 contains a time code generated by an internal clock in the ADC rather than data.

b. Tape Layout.

Each physical reel consists of 1 or more recording sessions of up to 1.14 hours each. Each session is preceded by a short identification record. The ID record consists of a 12-octal digit ID number repeated 8 times. This ID number is generated by a set of 12 octal switches on the ADC which are manually set.

The 8-word ID record is followed by one or more data records. Each data record consists of 6720 36-bit words representing 126 seconds of real time data. Following the data record is a 1 1/4" interrecord gap. The gap is generated by stopping the ADC without stopping the tape and represents a loss of 2 seconds worth of data out of each 128 seconds of real time.

The last physical record in the session is followed by an end of file mark. The last end of file mark on the reel is followed by an ID block with an ID number of all sevens, (777777777777).

c. Data Sample Packing and Interlace.

Each data sample consists of 12 bits, 11 bits plus a sign bit, thus each sample is a number limited 2048 > sample > -2048. Samples are packed 3 per computer word. Sampling of data channels proceeds in "frames"

of 1 second each, the pattern being repeated once per second. A tape record is 126 frames or 6720 words long. Each frame is sampled as follows:

 1
 2
 3
 4
 5
 6
 7
 8
 9
 10
 11
 12
 13
 14
 15
 16

 1
 2
 3
 4
 5
 6
 7
 8
 9
 10
 17
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 19
 20
 21
 22

 1
 2
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 14
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 16

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 4
 5
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 7
 8
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 12
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 14
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 16

 1
 2
 3
 4
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 7
 8
 9
 10
 11
 12
 13
 14

Sampling procedes from left to right. When read into the computer starting in location 1 the following pattern results:

		Samples in Bi	t Positions
Word	<u>S-11</u>	12-23	24-35
00001	1	2	3
00002	4	5	6
00003	7	8	9
00004	10	11	12
00005	13	14	15
00006	16	1	2
00007	3	4	5

etc.

4. Time Codes.

The time codes generated by the A/D converter and written on the tape as data samples for channel 30 are slightly different from ordinary samples in that they are unsigned 12-bit intergers. The clock counts in 1-second intervals from 0 to 4095 and counts modulo 4096.

The first time code on the tape in a session is 3, the last time code in the first physical record is 128. The interrecord gap represents two seconds, i.e., 129 & 130, thus the first time code in the second physical record will be 131.

5. Variations From Standard IBM Tape Format.

Tapes produced by the ADC while entirely compatible with IBM

729 Model IV or 729 Model VI tape drives have, none the less, certain variations from standard IBM formats.

- (a) Density Tapes are recorded at 512 rather than 556 bits/inch.
- (b) Interrecord gaps Interrecord gaps between data records are 1 1/4" rather than 3/4". The gap after the 8-word ID block is approximately 79". (The ADC produces only 6720 word records. Even though the ID block is only 8 words long, it writes enough blank tape to make a 6720word record).

3. Software.

a. Overview.

This section deals with the computer programs*. The programs as described are operational at the General Motors Technical Center computing laboratory. Since, however, their monitor system is unique, the programs as now written cannot be run directly on other 7094 installations. Mr. Singer and Mr. Stahlke in collaboration with the personnel at the NASA Ames Computing Center modified the programs so they can be run at NASA Ames Research Center. To run the programs at other computing centers would usually involve still other modifications as required by each local installation. If the programs were to be applied to different data tape formats, modification of the input routines would be required. The cards and listings for the operational programs may be obtained from The Lafayette Clinic, attention A. F. Ax.

The programs were designed to automate the analysis of physiological

* Programming was done chiefly by Samuel Singer with the help of Rudy Stahlke, Barbara Levin, Robert Hirschfeld, and James Licholat.

data by the use of a high-speed digital computer. A very large amount of data can be accumulated in a very short time in biological experiments in which many variables are studied simultaneously. The data acquisition system for which these programs were designed produces about a half million data samples per hour. Clearly this amount of data must be reduced to something more manageable by extracting only the most significant information, and perhaps equally important, it must be done at a reasonable cost.

With a problem of this magnitude it is important that the system as a whole be fast and efficient, yet it must be flexible to the greatest degree so that a variety of problems can be solved. Data storage was designed with minimum storage space and maximum speed of data retrieval in mind. Where compromises between speed and complexity were necessary, they were generally made on the side of greater speed.

The sections that follow describe the programs in some detail and also the logic involved in the choice of these particular solutions.

b. Points of Interest Program.

(1) The Response Concept.

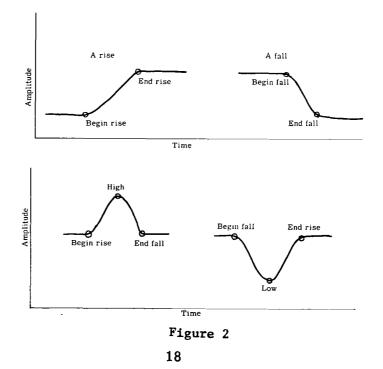
The data analysis is based on the concept of <u>biologic</u> <u>response</u> (Ax, 1958; Ax, Singer and Zacharopoulos, 1962; Ax, Singer, Zachary, Gudobba, and Gottlieb, 1964), which may be defined for any variable as a significant change in amplitude within a specified time limit. The question which must next be answered is, what is a "significant" change? Since there is a certain amount of "noise" inherent in any system, the amplitude of change must at least exceed the noise level and since there is a certain amount of homeostatic drift in amplitude with time, we may

realistically say the significant change in amplitude must occur within a certain time limit. The response is therefore defined in terms of two tolerances, an <u>amplitude tolerance</u> and a time or <u>duration tolerance</u>. A slope could not be used for the tolerance since noise may have high slopes. A response is an amplitude change that occurs within a duration tolerance and exceeds an amplitude tolerance.

A response may be either an increase in amplitude, a <u>rise</u>, or a decrease in amplitude, a <u>fall</u>. It begins when the variable changes amplitude by more than an amplitude tolerance within the period of one duration tolerance and ends when the variable no longer changes amplitude by more than an amplitude tolerance within the period of one duration tolerance. Since one response may immediately follow another, we must also say that a response ends when it changes direction.

(2) Points of Interest.

Responses are identified by their end points which are called Points of Interest (PI). The points are named according to the response they delimit. Examples (Figure 2) are Begin Rise (BR),

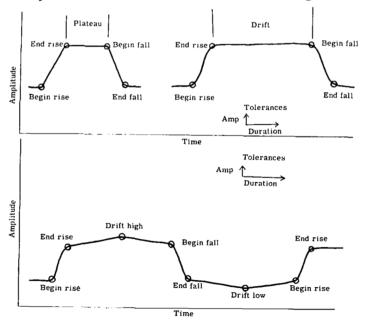


End Rise (ER), Begin Fall (BF) and End Fall (EF). The figures illustrate examples and Table 1 lists all points and their abbreviations.

Types of Points	Abbr.	Comment
Begin Rise	BR	CURV Computed
End Rise	ER	CURV Computed
Begin Fall	BF	CURV Computed
End Fall	EF	CURV Computed
High	HI	CURV Computed
Lou	LO	CURV Computed
Drift High	DH	No CURV Computed
Drift Low	DL	No CURV Computed
Begin Epoch	BEP	No CURV Computed
End Epoch	EEP	No CURV Computed
Begin Edit	BE	No CURV Computed
End Edic	EE	No CURV Computed
Begin Short Edit	BSE	No CURV Computed
End Short Edit	ESE	No CURV Computed

Table 1

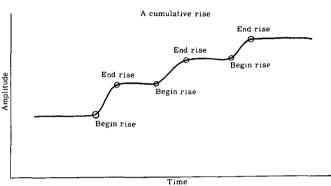
For the case in which one response does not immediately follow another, the portion of curve between two responses is known as a <u>drift</u>; and if the drift is of less than two time tolerances in duration, it is called a plateau. Examples of these cases are shown in Figure 3.





A drift may be of any duration. If during a drift the amplitude exceeds both end points by an amplitude tolerance, the extreme is identified as a <u>Drift High</u> (DH) or <u>Drift Low</u> (DL). A cumulative response consists of two or more discrete responses separated by plateaus (see Figure 4), but not by drifts.

The amplitude of a cumulative response is measured from the first begin rise to the last end rise.



Data are

Figure 4

generally recorded within a certain experimental design. The recording period is divided into one or more experimental epochs. It is usually desirable to identify the limits of an experimental epoch. This is done with special points of interest called <u>Epoch Points</u> (EP). These may or may not coincide with one or the other points of interest.

The points of interest are written on magnetic tape ordered by variable number in ascending time sequence. Each P.I. consists of (1) variable number, (2) amplitude, (3) time, (4) type (Hi, Lo, ER, etc.) and (5) curvature. These 5 values for each P.I. are packed into two words on the P.I. tape.

(3) Curvature.

We have now arrived at a set of parameters called Points of Interest which describe a curve. They have the virtue of being easy to obtain rapidly and of describing many important features of

the data concisely. One disadvantage of the Points of Interest is that they describe responses (our primary interest) only at their ends and say nothing about what happens between. Further information can be obtained as is illustrated by the cases shown in Figure 5.

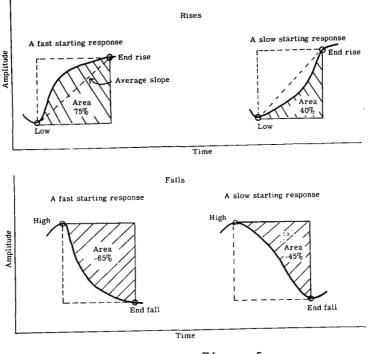


Figure 5

The first two responses shown have similar end points but different behavior in between. In one sense we might call the first a big response or fast-starting response and the second a small or slow-starting response. The area under the response, shown cross-hatched, is a good index of the difference between the two responses. A fast-starting response has a large area. The area is a way to describe the average curvature. Areas larger than the triangle enclosed by the average slope line indi-

cate a generally convex curve produced by a "negative acceleration" over most of the curve. Conversely areas less than the triangular area indicate a generally concave curve. To preserve this property of a fast-starting response being associated with a large area the complimentary area, or area over the curve, is computed for falling responses. In order to give the area or curvature concept a standard meaning regardless of amplitude, duration or area of the particular response, the percent of the rectangle encompassed by the amplitude and duration of the response is computed as illustrated.

(4) Artifacts and Editing.

Unfortunately real data generally contain a number of artifacts (noise) which must be handled in the data analysis. Indeed, to be generally useful the analysis system should be able to process data that are mostly artifactual and extract what good data are present.

Artifacts may be divided into two groups, those which can be recognized and interpolated or skipped by the computer and those which must be deleted by a human editor. In this system the computer recognizes as artifact those data which exceed either a specified amplitude or a specified slope. These two artifact tolerances are provided by the editor and provision is specified by a third editing tolerance, the <u>edit duration tolerance</u>. An edit of duration less than the edit duration tolerance is linearly interpolated. An interpolated edit is called a <u>Short Edit</u> (SE) while a longer noninterpolated edit is called simply an <u>Edit</u> (E). Their end points are special points of interest and are named <u>Begin Edit</u> (BE), <u>End Edit</u> (EE), <u>Begin Short</u> <u>Edit</u> (BSE), <u>End Short Edit</u> (ESE), as is appropriate. Examples of editing are

22

the section sector to

shown in Figure 6.

We have now briefly described the essential features of the first part of our data analysis system, the part called the <u>Points</u>

of Interest Program (Figure 7). This program which comprises the major part of the system can process several experimental recording sessions sequentially. It can handle 29 different channels of data simultaneously at 3 different sampling frequencies. It has provisions for scaling and converting data to physiological units as well as the features already described. Running time on the IBM 7094 for processing an hour's worth of data (about 500,000 samples for 29 variables) is about five minutes. A sample of

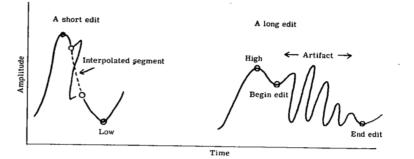
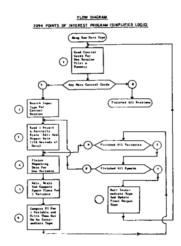


Figure 6





the polygram (Figure 8).

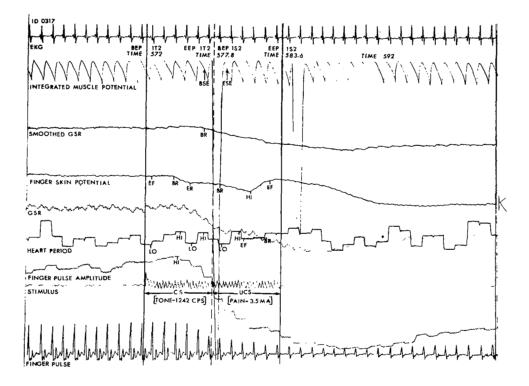


Figure 8

The raw data for all variables (Table 2, appendix) and Points of Interest and summary listing for the sampling of the variables are shown in Tables 3 to 12, appendix..

c. Summary Program.

The Points of Interest Program describes the data in terms of responses. While this considerably reduces the amount of data, the information is not yet organized into a form that is easily assimilated. The summary program is designed to perform the part of this function that does not require elaborate statistical analysis.

The summary program summarizes data by the experimental epochs which

were set up in the design of the experiment. It allows easy comparison of one epoch with another by summating the data. The summary tabulates separately three general categories of data: (1) general information about the epoch, (2) information about the first few responses in the epoch, and (3) a summary of various aspects of all responses for the entire epoch (Table 12a).

Ì

		POINTS OF INT	FREST SUMMAPY						
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	9EG FOTCH HEG AMP END AMP MAX AMP MTN AMP MFAN AMP	597.7 250.69 1261.65 1140.99 371.79 1200.36	FNN FPNCH 47 TIVF 47 TIVF 47 TIVF 47 TIVF 5144 NF	507.7 894.9 894.0 671.1		DUPSTION	300.3		
98.2	PER CENE (DOD	1414	1.6 YER CENT	1086 6011		פרב רדאד ל	400 7 50 T		
FIRST INTERVAL Response 1 Response 3 Response 3 Response 4 Response 4 Response 5 LAST INTERVAL	N T AMP 999.59 779.77 482.17 1771.62 979.72 1125.99	INCREMENT -21.77 -94.44 214.91 -195.47 148.96 -214.73	DUP 41 [02 2 , 3 2 , 5 3 , 4 2 , 1 4 , 1 6 , 1 6 , 1	51 'JDF -9,20 -44,23 -1,31 -64,01 74,03 -52,46 -52,46	1PF1 ,67 ,61 -,47 -9,37	(ATFHFV	9860 98157 ^. 7.7 7.7 7.0 0.		
	ç	UMMANY OF RES	PONSES, PLATENU	S. AND OWIETS	;				
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Table 12a

Each variable is summarized separately. The Summary categories are discussed in more detail below. (See Tables 4, 6, 8, 10, 12, appendix, for computer listing of the summary output for the data whose P.I. were illustrated.) Table 12a is an example of a standard summary output, but of different data.

(1) General Information Section.

This tabulation permits identification of the epoch and quick evaluation of the range of variation of the variable. It also gives some idea of the amount of useful information extracted by listing the number of points of interest in the epoch and the amount of editing. The following information is listed:

- (a) Variable Number.
- (b) Data Information Number.
- (c) Number of P.I. in Epoch.
- (d) Epoch Number.
- (e) Epoch Duration.
- (f) Epoch Beginning Time and Amplitude.
- (g) Epoch End Time and Amplitude.
- (h) Maximum Amplitude and its Time.
- (i) Minimum Amplitude and its Time.
- (j) Mean Amplitude and its Standard Deviation.
- (k) Percent Good Data.
- (1) Percent Long Edits.
- (m) Percent Short Edits.
- (2) First Responses Section.

Experimental epochs are usually set up to study responses to specific stimuli. The largest and most significant responses often occur immediately following the start of the epoch. In order to be able to examine the first part of the epoch indetail, the first few responses are tabulated individually. Up to 10 responses

may be tabulated for a given epoch as well as the first and last intervals in the epoch. The first interval is the period between the start of the epoch and the beginning of the first response and the last interval is the period between the end of the last response in the epoch and the end of the epoch. For each response and interval the following information is tabulated:

- (a) The initial amplitude.
- (b) The amplitude of increment or decrement.
- (c) The duration.
- (d) The mean slope.
- (e) The curvature index.
- (f) The latency time from start of the epoch.
- (g) The preceding drift time between the end of the

last response and start of the present one. The last item, preceding drift, is included to permit ready identification those responses that follow other responses immediately and those separated by drifts.

(3) Summary of Response Parameters Section. (Table 12a.)

This third section of the summary listing (which was not printed out in the preceding examples) tabulates the means and standard deviations of several aspects of the responses in an epoch. Data are tabulated separately for rises, falls, plateaus and drifts. The program also computes cumulative responses if they are present. Cumulative rises and cumulative falls are tabulated separately as well as the mean and standard deviation of discrete responses,

including those in cumulative responses, for each cumulative response.
For each discrete response, cumulative response, drift or plateau,
the number of each type plus the means and standard deviations for
the following parameters are tabulated: (a) increment or decrement;
(b) duration; (c) slope; (d) curvature: (e) interval between responses.

4. Program Input and Output.

The input to the program consists of the session identification numbers for the sessions to be processed, the variable numbers and the begin and end times for each epoch. The data input is the points of interest magnetic tape produced by the Points of Interest Program. Output is printed with an option of writing most of the printed output on tape for future statistical analysis.

d. Correlation Program.

(1) Unconfounded Parameter Correlation.

A method has been developed for correlation of the primary parameters of selected pairs of responses from a single variable or from pairs of variables. It does not employ the conventional auto- or cross-correlation approaches which utilize arbitrary equal interval samples; but rather this novel approach utilizes the time, amplitude, slope and curvature of the responses matched on the basis of minimal variance in lag.

This approach is not only parsimonious in computing time, because a highly selected and much reduced set of points is used, but also it has theoretical value. Consider these two variables in

Figure 9.

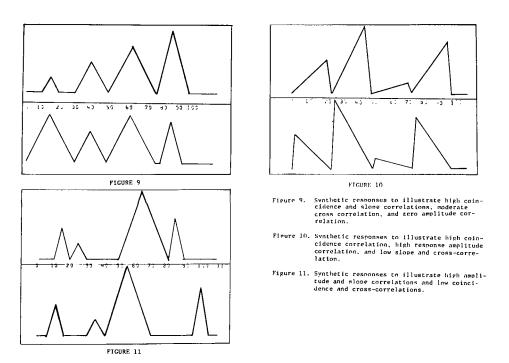


Figure 9

Would you say these two variables are correlated? Note that every time one variable rises to a peak, so does the other, reaching the maximum at exactly the same time. Thus, in the most primitive sense they are perfectly correlated by virtue of their perfect coincidence. We note also that the corresponding responses have exactly similar shapes; in each case the slopes of rise are the same and the slopes of fall identical on the two variables. Thus, their slopes are perfectly correlated. Their maximum amplitudes, however, are completely uncorrelated; the product moment correlation coefficient of their maximum values is exactly zero. The standard cross-correlation over time applied to these two variables produces a maximum correlation of approximately 0.57 for a lag of zero and less for all other lags. Since a correlation of 0.57 represents about 32 per cent of common variance, we could conclude they are weakly correlated by this classical correlation function; their maximum amplitudes are completely uncorrelated but they are perfectly correlated by indices of coincidence and slope. In the next example (Figure 10) the two variables, when adjusted for lag, have perfect product moment amplitude correlation of their maxima, perfect consistency in lag, but by virtue of their differing shapes produced by differing rise and fall slopes the maximum cross correlation is a minute 0.35 with an optimum time lag of 15.

Finally in Figure 11 the two variables again have responses of perfectly proportionate amplitudes, itendical shapes but this time inconsistent lags. The maximum cross-correlation whuch occurs at lag 10 is only 0.20.

These examples should make it clear when dealing with variables which have irregular intervals and variable shapes due to different rise and fall slopes, that none of the conventional methods of correlation gives a full and unambiguous measure of their correlation. The standard crosscorrelation function based on equal interval samples correlated over a mean time lag (Tau) clearly produces some cort of average, confounded of all three aspects of coincidence, amplitude and slope. In biological systems it may be important to measure any one of these three aspects of correlation independently according to its own internal principles of response. Classical cross-correlation in this situation would reveal only a weak relationship, whereas control may be absolute with regard to <u>occurrence</u> and <u>timing</u> of the dependent systems' response. The neural

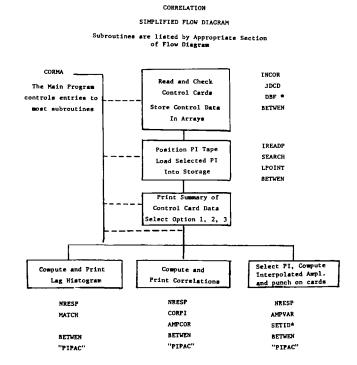
impulse which starts the heart beat is this type of response.

In attempting to apply standard cross-correlations to respiration produced heart period variability called "respiration simus arrhythmia" we have often found small "zero-order" correlations in respiration and heart rate records which by visual inspection, appeared to have strong sinus arrhythmia. These inconsistent findings stimulated us to seek better ways to measure cross-correlation among physiological variables.

Our approach keeps entirely separate the aspects of coincidence, amplitude, and shape. It retains the concept of a response as the primary entity. The first problem is to identify the corresponding responses on a pair of variables.*

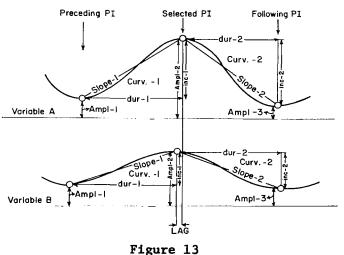
(2) Phases of the Correlation Programs.

The correlation of response parameters proceeds in two Matched PI For Correlation distinct phases (Figures 12, 13, 14).



* GH System Subroutine. "PIPAC" is a FAP coded routine with multiple entries for packing and unpacking parts of PI.





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- * Ax, A. F.; Zachary, G.; Gudobba,
 - R. D.; Gottlieb, J. S.

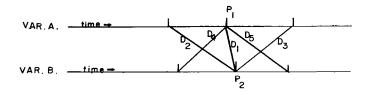
Psychophysiological data

retrieval and utilization.

<u>Ann. N. Y. Sci.</u>, Vol. 115:

2, pps. 890-904, 1964.

CORRELATION MATCHING METHOD



The PI are indicated by short vertical lines on the time scale of the two variables. P_1 will be matched with P_2 if the time differences D_1 through \hat{D}_5 meet the following test: D_1 must be less than D_2 , D_3 , D_4 , or D_5 .

During the first phase, the times of selected P.I. are matched and a histogram of the lags between samples for the pairs of variables being matched is printed out. This enables the user to select the characteristic

Figure 14

lags for the P.I. he desires to correlate. During the second phase these lags are used as input. The selected P.I. are matched and the subset of those points closest to the specified lags is used for the actual correlations. Matching may take place on either the beginnings or ends of responses as desired.

The input to the program is similar to the P.I. and summary programs previously described and consists of a set of program control cards specifying the desired program parameters and a tape containing the points of interest in the format produced by the P.I. program. Output consists of a summary of control card information plus identification data such as epoch and variable names from the P.I. tape. This is followed by the lag histograms for phase 1 and correlations for phase 2 in convenient tabular form. The program contains extensive optional printout of intermediate data for use in checkout and during early program usage. III. APPLICATION OF ACQUISITION SYSTEM.

The data acquisition system became operational long before the data processing system did. During this time, considerable data were recorded

by oscillogram and analog magnetic tape. Three physiological variables were analyzed by hand on two studies. The first of these studies has been partially reported previously. (See Ax, Beckett, Fretz, Gottlieb, 1965.)

- A. Classical Conditioning of Autonomic Responses in Humans.
 - 1. Rationale.

The notion underlying this study is the concept of learned moti-It is well established that the motives which the individual develops vation. by interaction with his social environment are learned, (Hull, 1943; McClelland, Atkinson, Clark, & Lowell, 1953; Hebb, 1958; Brown, 1961; Miller, 1951; Miller, 1961). The individual learns his motivational pattern uniquely according to his particular endowments and experiences. Since there is almost always more than one motive present, it is necessary to conceive of motives as being organized into a hierarchy in reference to current need, opportunity, and long term consequences. Current need, opportunity and long-term consequences, are very interdependent variables which may interact strongly as illustrated by emotional behavior and impulse buying which after the act may be seen as very inappropriate behavior and to result in undesirable long-term effects. The motivational hierarchy which enables the decision to act (presumably by some sort of reciprocal inhibition) is largely unconscious and may have little relationship to the verbalized conscious "hierarchy of values".

One who tends to be overweight may have placed dieting high on his verbalized hierarchy of values but continue to overeat. The motive to diet is obviously not very high on his hierarchy of motives. This common difficulty in human motivation can be seen to be largely due to the relatively low potency for some people of long-term--as contrasted to short-term--reinforcements. An immediate threat to health is usually quite successful

for dieting. Clearly to predict and understand behavior the true hierarchy of motives rather than the deceptive verbal "hierarchy of values" must be studied. It is for this reason that the unconscious involuntary physiologic processes are used to study motivation.

The motivational aspect of behavior is believed to be managed by the limbic system of the brain which regulates the autonomic nervous system (ANS). The physiological functions controlled by the ANS thus are prime targets to study with regard to their role in learning motives.

The concept of an aptitude for learning the hierarchy of motives seems strange to some people. Yet few would doubt that the establishment of the hierarchy is learned. Wherever there is learning, we may postulate, there must be an aptitude for the learning. All aptitudes that have been measured appear to be widely distributed in the population and are in general only moderately correlated with each other. Thus we do not expect fo find musical talent, verbal ability and athletic ability to be highly correlated; similarly the aptitude for learning the social motives need not be well correlated with the well-studied aptitudes mentioned above.

Just as educators know that they must adapt their procedures to the intellectual abilities of the student and adjust their expectations for him in terms of his I.Q., so must we learn to recognize and measure the aptitude for learning the social motives and to adapt our social incentives to the person's motivational aptitude and to adjust our expectations of his achievements in terms of his aptitude for learning the social motives.

The aptitude for learning the social motives has a general effect on all achievement, since motivation is a prime factor in all behavior. No matter

how great the talent, if motivation is low there can be little achievement. It would appear that motivational learning is influential for its own acquisition in a regenerative, positive feedback way, thus playing a power factor role. From early childhood relatively small differences in initial motivational aptitude may have profound effects on achievement.

Successful demonstration that these physiological measures of learning correlate with motivational aspects of important life activities such as education, work and family responsibilities would contribute to better scientific description of the mechanism of motivation and to the practical application in selection and training of personnel.

2. Method.

This was a study of clinical group differences rather than one of conditioning per se, hence identical procedure was used on all subjects rather than a procedure employing methodological subgroups for control of stimulus order, pseudo-conditioning, etc. This orientation to clinical group differences makes the study less than ideal for the analysis of the nature of the conditioning obtained. Subsequent studies will be required to clarify these interesting problems.

a. Experimental Procedure.

The experiment was done on each subject over a 5-day period (Figure 15 next page). Five 1-hour sessions of physiological testing were done on consecutive days. The first session was habituation to the laboratory during which 3 different pitched tones were sounded each for 12 seconds for each of 5 trials. The second and third sessions were for conditional training during which two of the tones were reinforced by two different intensities of pain stimuli each 5 times per session. The fourth session

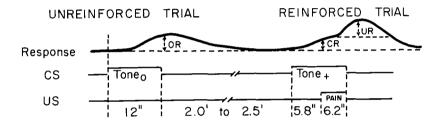
CONDITIONING PARADIGM

DAILY SESSIONS

Habituation Ist cond. 2nd cond. Extinction Cold Pressor

A CONDITIONING SESSION







was extinction during which only the tones were given as on the first day. At the completion of the extinction series, the pain electrodes were once more attached and 4 intensities of stimulation (2.5, 3.5, 4.0, and 4.5 ma) were administered at about 3.0-minute intervals so as to enable the determination of the subjects' responsiveness to the pain stimuli when the response was not complicated by a preceding CR elicited by the CS. It was hoped that these responses could be used in a regression equation to adjust for individual differences in response sensitivity so as to reduce the betweensubject variance. The pain stimuli can also reveal the systematic discrimination of the response system to incremental pain stimuli.

On the fifth day the cold pressor test was done and 3 I.V. blood samples taken for biochemical analysis being done by Dr. Frohman. The experimental

procedure for each session was preceded by at least 5 minutes recorded undisturbed rest and followed by a 5-minute rest period.

The conditional stimuli used in this experiment were tones of 3 different pitches (470, 770, and 1240 Hz) interrupted (50% on - off 4 times per second at about 75 db loudness. Each tone was presented for 12 seconds for 5 repetitions at pseudo-random intervals (from 2.0 to 2.5 minutes) in 4 sessions on consecutive days. The unconditional stimuli were direct currents applied to the toe pads via zinc sulphate wetted circular sponge electrodes. The direct current values were 2.5 and 3.5 ma; that is, 6.50 and 9.10 ma/cm². An electronic current regulator maintained precisely these current values regardless of skin resistance changes beneath the electrodes. During the first or habituation session each of the 3 tones without the pain was presented 5 times. During the second and third sessions the smaller (2.5 ma) pain stimulus always accompanied the last 6.2 seconds of the middle pitched tone (770 Hz) and similarly the higher pain stimulus (3.5 ma) was always paired with the highest pitched tone (1240 Hz). The lowest pitched tone was never reinforced by pain. On the fourth or extinction session no pain stimuli, only the tones, were presented. This session was identical with the habituation session. Thus during the two conditioning sessions each of the two higher-pitched tones was reinforced a total of 10 times.

Each subject was told for the habituation session that he would hear some tones but he need do nothing. For the two conditioning sessions he was told that some of the tones would be accompanied by a brief pain in his toe which would feel like heat. For the 4th or extinction session he was told that there would be no pain stimuli--that the pain electrodes were not applied to his toe. This true information was given to the subject

in the hope that it would eliminate the random variance caused by varying hypotheses of the subects as to when they might be given pain stimuli. The involuntary autonomic response was of more interest than the conscious expectations.

On the fifth day the subject was required to immerse his foot in continuously stirred ice water for 1 minute. I.V. blood samples were taken before, during, and after the ice water stimulus. During the 10 minutes of stimulation, the maximum rise and fall from the prestimulus resting levels were scored for each variable.

b. Subjects.

Three types of subjects were tested:

(1) The clinical group consisted of 28 male chronic schizophrenic patients with an age range of 27-41 with a mean age of 31.9 years. The mean duration of the illness was 7.6 years with a minimum of over 2 years. They were maintained in a special research ward and kept off all drugs for a year or more prior to the time of testing. They were on a good diet and required to participate in a daily program of exercise. According to the diagnosis by a single psychiatrist on a single occasion, their subdiagnoses were distributed as follows: Paranoid 36%, Hebephrenic 18%, Catatonic 14%, Simple 14%, and Undifferentiated 18%. During the 8 years most of these patients have been studied, there have been changes in psychiatric opinion about their subdiagnostic categories; all clinicians agreed, however, that all 28 patients were indeed chronic schizophrenics.

(2) The control group consisted of 18 healthy employed persons. Each was interviewed by a psychiatrist and rated on the same psychiatric scales on which the patients were rated. In addition the control group was given the Minnesota Multiphasic Personality Inventory, the Wonderlick

Personnel Test, a reversed digits test, and weight and auditory discrimination tests. If any control subject was judged to be unhealthy physically or psychiatrically by the psychiatrist, he was excluded from the control group. The age range was 19 to 44 with a mean age of 28.1 years. There was no attempt to match the two groups on I.Q. Within the control group there was no significant correlation between the GSR conditioning score and the Wonderlick index of I.Q.

c. Physiologic Response Scoring.

Manual analysis was done on skin conductance (SC), skin potential (SP) and finger pulse (FP). The analysis of heart rate, respiration, frontalis muscle tension, face temperature, and ballistocardiogram was postponed until computer analysis could be done.

(1) Base Level.

The palmar conductance and potential were measured prior to the onset of each stimulus and also at five selected points of each (a) During the last minute of the first rest period.

- (b) Between the 5th and 6th stimulus (at the lowest SC point and point of least activity of SP).
- (c) Between the 10th and 11th stimulus.
- (d) Between the 15th stimulus and the instructions for rest.
- (e) Near the end of the final rest period.

Since finger pulse had no calibration, the base level was not considered a useful measure.

(2) The Conditional Responses (CR) to tones (T, T, T)0 1 2 were measured during the habituation and extinction sessions within the 12-

second period while the tone signal was on. During the conditioning sessions the CR was measured only during the 5.8 seconds of the tone prior to the onset of the pain stimulus. The responses to T_0, T_1 , and T_2 were each measured in the same manner during the conditioning sessions, except those for FP for which the T (unreinforced tone) was measured over the full 12-second tone interval as it was for all variables during habituation and extinction sessions. The purpose of this change was to enable, for one variable, a proper comparison between the unreinforced and reinforced sessions which is not possible when the periods of analysis are of different length. The more obvious solution to this problem would appear to have been to have measured all responses to tones for all sessions only during the first 5.8 seconds of the tone. If this had been done comparisons between tones and between sessions would have all been possible. The reason it was not done was because many of the responses, especially those of FP, had rarely reached their full amplitude at the end of the 5.8 second period; hence, the value obtained at the 5.8 second cutoff was not the best representation of the response amplitude. The data should be rescored both ways to test this hypothesis and to enable all comparisons. Another experimental design which employed unreinforced trials for the usually reinforced tones, T and T, would, of course, also have provided a solution. This was not done because we feared that less than 100% reinforcement would produce inadequate conditioning in this experiment where the total number of reinforcements was only 10 per tone. Finally it must be reiterated that our primary purpose was the group comparisons rather than a study of conditioning.

(3) The unconditional response (UR) was measured during the 6.2-second period while the pain stimulus was on. In order to make the CR and UR comparable the UR analysis period was not carried beyond the offset

of the pain even though many responses continued to rise after the US offset. The UR are being rescored to examine the full response.

Another problem in comparing the CR and UR is the fact that the UR is nearly always occurring during some phase of CR response or recovery. As mentioned earlier the "Law of Initial Values" is not sufficiently sophisticated to enable correction for this aspect. For some variables and for some stages of the just previous response, the second response may be augmented; for other variables and stages, it may be diminished in amplitude. John Gorham working in our laboratory is investigating this problem.

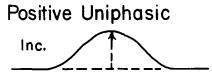
All responses are calculated by subtracting the amplitude just prior to the beginning of the response from the value either at its maximum or at the end of the analysis epoch as described above.

Skin potential (and heart rate when it is analyzed) presents special problems because it has four typical patterns of response: (a) positive uniphasic, (b) negative uniphasic, (c) positive diphasic (positive portion first), and (d) negative diphasic (negative portion first). The polarity of the response is the potential at the palmar surface referenced to the arm electrode. Normally the palm is negative to the arm reference. No special procedures (such as skin drilling) were used to decrease the resistance at the arm site except the usual washing and rubbing in of electrode paste (Redux). Variable resistance effects between the electrodes and loading was prevented by using an electrometer coupler having over 1000 megohms input impedance. We have determined that at least 10 megohms input impedance is necessary to prevent loading and resistance effect.

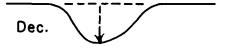
The SP measures were taken as follows: (a) frequency of each type, and (b) amplitude of the increments and decrements from both types of responses

whether from uni- or di-phasic responses. In order to avoid scoring as responses the recoveries, only that portion of the secondary wave which exceeded the beginning amplitude was utilized as illustrated below in Figure 16.

Types of Skin Potential and Heart Rate Responses



Negative Uniphasic







There are problems which require arbitrary solutions. (1) For a response to be counted the change for this study must be at least 0.2 mv in amplitude within 1.0 second. For SC the change must be 0.05 micromho within 5 seconds. (2) If the recovery of a response is not completed when another response of the same polarity occurs the second response must be treated as another response. If the second response reaches a greater value than the first one

(all within the specified analysis epoch), the maximum value of the second response may be used as the minuend from which the amplitude of the variable at the beginning of the first response is subtracted to produce the response amplitude. Such a response is called a cumulative response. (3) The remaining arbitrary consideration is the maximum interval between the maximum or end rise of the first response and the beginning of the second response so as to distinguish between discrete and cumulative responses. This value has been set at twice the time tolerance. For SP it is 2.0 seconds and for SC it is 10 seconds. It should be emphasized that neither frequencies nor amplitude distributions are meaningful nor comparable unless such scoring standards are followed and stated.

There is as yet no clear understanding of the significance of these different types of skin potential responses. Chester Darrow (1964), Robert Edelberg and David Wright (1964), and R. C. Wilcott (1964) have presented tentative explanations but at present no generally acceptable explanation has been presented.

3. Results.

a. Base Levels.

The tendency for the schizophrenic group to have significantly (p < .05) higher average base levels of palmar conductance over all four sessions suggests a higher level of activation (Table 14).

BASE LEVELS*

Variable	Hab:	ltuation		irst itioning	Sec Condi	ond tioning	Exti	nction	4 5	essions	Cold	Pressor
	с	s	с	S	с	s	с	s	с	s	с	s
SC	2.71	4.18	3.29	4.29	3.54	4.27	2.54	4.03	3.03	4.19	2.63	3.57
SP	-2.6	-14.3	-17.2	-14.9	-18.0	-15.0	-15.8	-12.9	-14.11	-14.16	-	-
SBP	119.7	118.9	120.8	116.3	120.8	120.3	117.8	116.7	119.8	118.1	• 116.4	113.2
DBP	77.3	78.8	77.0	77.3	77.8	80.8	74.9	77.4	76.5	78.5	73.3	73.0

* Middle three samples for each session.

For controls Base Level $r_{sc.sp} = .26 \ p > .05$ (4 sessions) For Schiz Base Level $r_{sc.sp} = .28 \ p > .05$ (4 sessions)

Table 14

The two groups do not differ significantly on SP or BP. It is not known whether higher or lower skin potentials are associated with arousal. But since SP and SC for mean base levels have only insignificant correlations for both control (r = .26) and schizophrenic (r = .28) groups it would appear that SP is not an indicator of the same aspect of arousal that SC is believed to be.

Without valid base level measures for such additional variables as heart rate, peripheral plethysmogram, muscle tension, and EEG desynchronization it would be hazardous to say how the two groups compared on activation or how they adapted over the sessions. As Lacey (1966) has recently pointed out and Darrow (1942), Ax (1953), Sternbach (1960), Lazarus (1966), and others have shown, the physiological indices of activation do not correlate very well. We conclude that activation or arousal is too global and undifferentiated a concept accurately fit the facts. Individuals manifest their activation in unique patterns and do so differently in different situations. Much more research is needed to relate patterns of physiological activation with well described emotional and motivational patterns in many types of individuals.

The correlations between base levels and the various indices of response show a similarly variable pattern. Of the correlations computed on individuals for SC between base levels and response, the range was from zero to .74. For SP they are equally variable. Such wide individual differences and variability within individuals in regression of response amplitude on base level makes questionable any attempt to remove the base level contribution from response amplitude. There is little to be gained by attempting to apply the "law of initial values", until studies are done which sufficiently

control for the other determinants of response amplitude. The determinants other than base level include individual response specificity, type of arousal and contribution of other variables. Many studies must be done to reveal the true, probably curvilinear, relationship between response amplitude and base level for each variable, each type of stimulus and each "type of subject" (if indeed each individual is not a type unto himself). We come to this lamentable conclusion even though we believe that the contributions of psychophysiology to the study of stress tolerance, motivation and emotional development can be greatly enhanced by the full exploitation of the true "laws of initial values." Much research needs to be done in this area.

b. Orienting Responses.

An important consideration for classical conditioning is for the conditional stimulus originally not to elicit much of an orienting response, or at least to be relatively habituated, before conditional training is begun. Minimal response to the CS prior to conditioning makes it easier to show unambiguously that enhancement in response amplitude or frequency of response has been achieved by the training procedure. There is uncertainty as to exactly what role the amplitude of the OR has for the course of conditioning. Often it is found that for pseudo-conditioning control groups where there is no pairing of CS with UR the OR habituates whereas for the conditioning groups the OR does not habituate and is said to have become the CR. Some experiments have described increases in latencies as OR became CR and others have even described a third response called the anticipatory response, AR, which occurs just before the US. These varieties of responses are probably influenced by the duration of the CS-US interval, latencies of the response variable, etc. Since our primary

purpose was to describe the differences between two criterion groups rather than detail the intricacies of classical conditioning, we can pursue this problem no further. It is sufficient to note (see Figures 17 to 24, next page) that the healthy control group had larger OR at the beginning of the habituation session but that at the end of the habituation session their mean OR was no larger than that for the schizophrenic group. Thus the conditional response differences between groups cannot be accounted for simply in terms of larger responses to the CS prior to conditioning nor by the OR since the correlations between OR and mean CR are small, averaging .27 for the control group and .21 for the schizophrenic group (Table 15).

ADAPTATION OF ORIENTING RESPONSES

		sc			FP			sp _i			sp _d	
	С	s	P	с	s	р	с	S	p	с	s	P
lst OR - Iast 3 hab.	. 373	.022	-	12.73	8.02	-	.029	.039	-	,281	.020	-
2nd Or - last 3 hab.	.244	.070	-	14.30	-5.01	-	.253	.004	-	.166	.007	-
Comb. OR - last 3 hab.	. 299	.034	۰.01	13.09	-2.11	.01	.122	.018	.05	.249	.014	.01

1st OR is the response to the first 3 tones of habituation.

2nd OR is the response to the first tone (T_) of first conditioning.

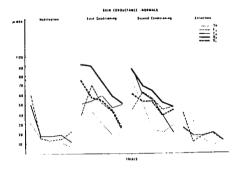
Combined OR is (1st OR + 2nd OR)/2.

Last 3 hab. is the mean of the responses to the last 3 tones of habituation $(T_1 + T_2 + T_3)/3$.

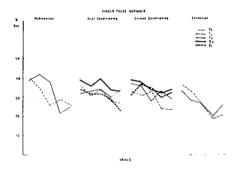
CORRELATIONS OF OR HABITUATION VS CONDITIONING

Table 15		SC	FP	SP;	SPd
	Control (N=18)	.363	.096	.691	.539
	Prob	NS	NS	.01	.05
	Schiz (N=28)	.413*	.137	.440	.018
	Prob	.02	NS	.02	NS
The OR habituation (Table 16) corre- lates with condition-	trial. The co	<pre>Habituation is ist trials/3 - 3 i, T1, 1st cond mditioning score second condition;</pre>	last trials/3 f E last 3 trial is the mean am	s/3 for habituat	ion).
ing on the average considerably better	* One subject caus non-parametric Rag				

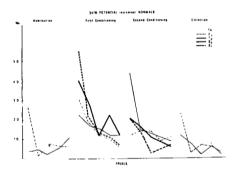
Table 16













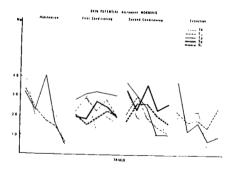


Figure 23

L

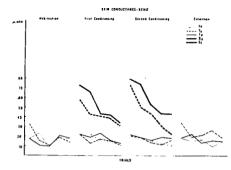


Figure 18

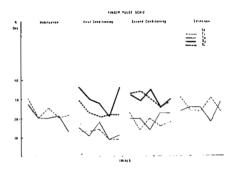


Figure 20

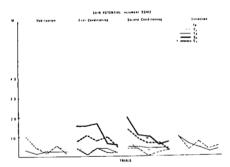


Figure 22

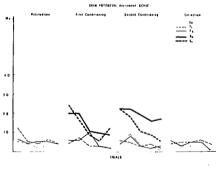


Figure 24

for controls (.419) than for schizophrenics (.252).

It could be that two factors are involved here. The higher initial OR for the healthy group may represent a greater sensitivity to their environment and their rapid habituation could be considered as conditioning. Conditioning in the general sense is <u>modification</u> of a response with experience and may include decreases as well as increases. The role of the OR ("sensitivity to stimuli not yet classified as to relevance") in conditioning is not well understood, although it could be argued that for a stimulus to become a successful conditional stimulus, it must be taken cognizance of (responded to) in some manner by the organism. It is unknown to what extent an organism will develop a sensitivity to a previously totally ignored stimulus by associative conditioning.

c. Unconditional Responses.

A second important consideration for conditioning is for the unconditional stimulus (US) to elicit an adequate unconditional response (UR). Reference to Figures 17-24 and Tables 17

				RESPON	ISE AMPI	ITUDES.						
		sc			FP			sp _i			sp _d	
CR	с	S	p*	c	5	p*	с	s	p*	С	5	p≢
Habituation Ist Conditioning 2nd Conditioning Ist & 2nd Condit. Extinction	. 21 . 49 . 54 . 52 . 20	.17 .16 .16 .16 .18	NS .01 .01 .01 NS	28.44 31.98 31.12 31.89 29.99	27.55 11.47 18.90 15.06 40.71	NS .01 .01 .01 NS	.68 1.58 1.58 1.67 .79	.50 .34 .41 .38 .50	NS NS .05 .05 NS	2.11 2.79 2.11 2.47 1.72	.55 .53 .48 .51 .42	.01 .01 .01 .01 .01
UR lst Conditioning 2nd Conditioning lst & 2nd Condit.	. 63 . 58 . 61	.47 .51 .48	.05 NS .05	32.59 33.82 32.56	24.60 31.34 28.63	NS NS	2.24 1.12 1.68	1.10 1.01 1.07	.05 พร พร	2.06 2.51 2.21	1.44 1.69 1.58	NS . 05 NS

Amplitudes for the habituation and extinction sessions are means of responses to all tones. Amplitudes for the conditioning sessions are means of the responses to the reinforced tones (T $_1$ and T $_2$), and means of the responses to the unconditioned stimuli (S $_1$ and S $_2$).

*Kruskal-Wallis one way analysis of variance.

Table 17

					PERCENT	RESPONS	E FREQUEN	сү					
and 18			sc			FP			sp _i		sp.		ı
	CR	С	S	p*	с	s	p *	С	S	n*	С	s	P*
shows that	Habituation	72.7	59.6	NS	70.0	65.9	NS	20.3	28.3	NS	67.1	39.3	.0013
	1st Conditioning	93.7	59.1	.00003	93.1	43.1	.00003	18.1	17.1	NS	81.2	39.9	.0004
	2nd Conditioning	91.7	61.2	.00016	89.4	63.3	.0011	24.2	18.5	NS	70.1	42.9	.0008
• • • • •	1st & 2nd Condit.	93.2	59.8	.00003	91.1	53.2	.00003	21.0	18.0	NS	74.3	41.3	.00004
both the	Extinction	66.0	61.1	NS	71.1	69.8	NS	20.5	28.0	NS	57.1	35.6	.0228
·	. UR												
amplitude	lat Conditioning	96.5	90.2	NS	94.6	78.6	.0217	35.0	23.7	NS	63.8	65.2	NS
····•	2nd Conditioning	90.9	84.5	NS	92.8	86.9	NS	24.4	27.3	NS	70.5	59.0	NS
	let & 2nd Condit.	93.7	87.6	NS	93.6	83.0	.0113	29.2	25.2	NS	67.8	62.2	NS
	IBC a zha conaic.	,	07.0	110	,,,,,	02.0	.0115	27.1	20.2		07.0	02.2	
and fre-					SKIN PO	TENTIAL	. SUBTYPES						
_		Posi	tive Un	iphasic	Pos	itive D	iphasic	Neg	ative Un	iphasic	Neg	ative I)iphasic
quency of	CR		с	s		с	s		с	s		с	s
	Habituation	18	.7	28.3	1	.6	o	5	2.6	33.3	1	4.5	6.0
IIP annoam	lst Conditioning	18		17.1		0	0	6	1.9	33.2		9.4	6.7
UR appear	2nd Conditioning	21		15.3	2	.8	3.2	4	6.0	32.5		4.1	10.4
	1st & 2nd Condit.	19	.5	16.3	1	.4	1.6	5	3.7	33.0	2	0.6	8.3
	Extinction	17	.4	27.5	3	.1	.5	4	7.6	30.0		9.5	5.6
adequate	UR												
		27		23.7		-	0		9.4	46.2			10.0
C	lst Conditioning 2nd Conditioning	33 20		23.7		.2 .9	5.2		9.4 9.4	46.2		4.4	19.0 14.6
for the	lst & 2nd Conditioning	26		22.6		.9	2.6		9.4 0.6	44.4		1.1 7.2	14.6
	ISC 6 2nd Condit.	20	. 4	22.0	2	.0	4.0	4	0.0	43.8	2	1.4	10.4
	Percent response fro	equency is	s the c	ercent of	possible	e respo	nses made	to all	three to	mes for I	be habi	tuation	,
two groups.	and extinction sess												
cao groups.	tones (T and T), a							,					

and extinction sessions. For the conditioning sessions the percent frequencies are those for the reinforced tones (T_1 and T_2), and for the unconditioned stimuli (S_1 and S_2).

No sub-

ject

Table 18

failed to provide UR. The correlations between parameters of CR and UR are very low (.01 to .21) which suggests that if some minimal UR is present, it suffices for conditioning.

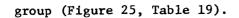
d. Conditional Responses.

*Mann-Whitney U test.

The most remarkable finding is the greatly reduced mean conditional responses for the schizophrenic group as shown in Tables 17 and 18. Appropriate probability tests of these group mean differences indicate it is highly improbable (p < .01) that these differences could be due to chance. The percent of cases correctly classifiable by these scores indicate several individual scores to be highly diagnostic, thus indicating the autonomic conditional approach may have considerable power as a diagnostic test.

e. Tone Discrimination by CR.

The response discrimination between the reinforced tones (T_1, T_2) and the unreinforced tone (T_0) shows essentially no discrimination for the schizophrenic group and only moderate discrimination by the normal



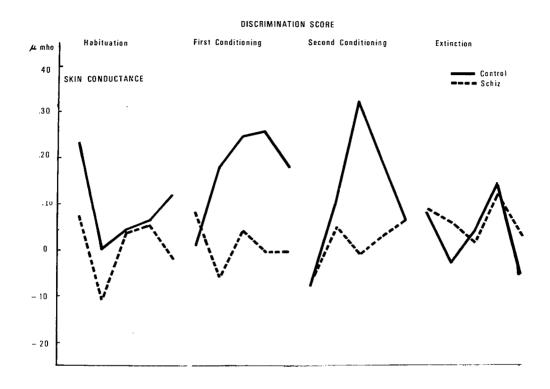


Figure 25

				DI	SCRIMIN	ATION SCOR	ES						
		sc		FP			SP.			sp_d			
	с	S		с	s		с	s		с	S		The curves do not
Habituation	.08	.01	.05	9.31	.17	.05	. 22	03	.05	.10	. 21	NS	
First Cond.	.17	.02	.01	-5.79	-6.07	NS	.08	.00	NS	. 58		.05	suggest any im.
Second Cond.	.11	.02	NS	-7.68	-6.37	N5	.11	07	NS	.18	0:	NS	
First and Second Cond.	.14	.02	.01	-6.52	-5.47	NS	.13	02	NS	. 38	.02	.01	provement in dis-
Extinction	.03	.05	NS	1.23	1.88	NS	01	.17	NS	.25	. 21	NS	crimination with
Discriminatio	on Scor	e = (T	, + Τ_)/ ,2	2 - T ₀									increasing trials
													after the middle
				Г	able	e 19							of the first

conditioning session. Any discrimination that had developed during the rein-

forced period promptly disappeared when reinforcement was omitted in the extinction session.

The significantly greater discrimination demonstrated by the control group shows that at least a part of the conditioning superiority of the control is due to discriminative learning and not mere sensitization as could be claimed for the greater frequency and amplitude of the CR since there was no control for pseudo-conditioning.

f. Variance in Latencies.

Still another measure of response to the CS is the variance in latency. If the responses of a subject have a significantly smaller variance than would be expected by chance to randomly selected periods where no experimental stimuli were given, it is demonstrated that at least some of his responses measured during the stimulus are elicited by the stimulus.

Since the latencies to an imaginary random stimulus would have a uniform random distribution the theoretical variance would be:

$$\sigma^2 = (\alpha - \beta)^2 / 12$$

where α is the lower boundary and β the upper boundary of the range. Since our conditional stimulus period was 5.8 seconds the theoretical variance is 2.83. It was found for GSR latencies of CR for 8 trials selected for best discrimination between groups by GSR CR amplitude that the 18 normal subjects had significantly smaller than chance variance in latency whereas only 13 of 23 of the schizophrenic patients had such small latencies (variances were not computed for five subjects who had less than three responses).

This finding suggests that about half of the patients were not responding to the tones significantly more than chance. One can confidently conclude that at least these subjects and those with too few responses did

not condition probably because their responsiveness to the CR was too small or inconsistent to enable conditioning. On the other hand those who had significantly smaller than chance variance in latency do not by that fact alone demonstrate conditioning. Their responses to the tones could mean only that they were continuing to make orienting responses to the CS with neither normal adaptation of the OR nor with any enhancement due to conditioning. Without additional control groups for pseudo-conditioning for which the CS and US are given but not paired, it is impossible to distinguish between "true conditioning" and sensitization or failure to habituate the OR. ı.

g. Combined Scores.

By combining several of the conditioning measures (Table

20,

I.

SUMMATED SCORES

	Σ React.	Σ Cond.	Σ Disc.	<u>Σ</u> CP	Σ Tot
Cont.	.459	.939	.505	. 715	.656
Schiz.	295	602	352	470	431
Diff.	.753	1.541	.857	1.185	1.087
Prob.	< .02	< .01	< .01	< .01	< .01
Reactivi	ty = (1) Mean	FP _{dec} and SC	nc to 4 pain sti	.muli at end of	extinction +

(2) Total FP and SC response to T₁, S₁ and T₂, S₁ for 1st and 2nd conditioning +

(3) FP decrement plus SC increment during CP session.

conditioning = SC + FP + SP_{dec} CR amplitude + FP_d % frequency for 1st and 2nd conditioning.

 $\begin{array}{l} {}_{\Sigma} \mbox{ Disc = (T_1 + T_2)/_2 - T_0} \mbox{ for lst and 2nd conditioning for SC and SP}_d. \\ {}_{\Sigma} \mbox{ CP = (HR_i + SC_i + BC_i) - (DBP_i + MT_i + \theta \mbox{ GSR) for Cold Pressor.} \end{array} \end{array}$

Table 20

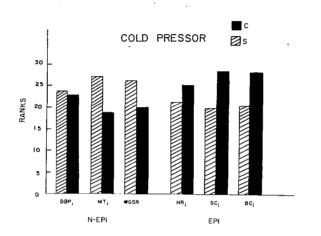


Figure 26

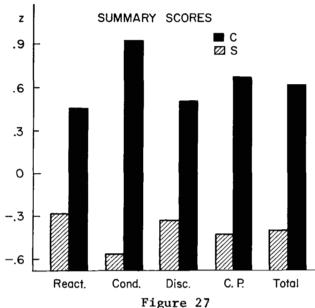
which best distinguish between the two groups it is possible to classify 87% of the total group correctly with only 3 normals and 3 patients misclassified. This is the same percent correct classification as for the single best conditioning score which implies that the autonomic conditioning is similarly reflected in all 3 variables. Probably much of the variance not common to these conditioning variables is due to error.

However if we add to the conditioning scores an index obtained from the physiological response scores to the cold pressor test (Table 21,

		REST			INC			DEC
	С	s	Р	с	S	Р	с	S p
HR	63.4	70.0		30.0	26.8		8.0	6.1 N.S.
SBP	116.4	113.2		- 17.6	21.3	N.S.		-
DBP	73.3	73.0		14.3	14.8	N.S.	-	-
BCG	. 79	.75		26.2%	16.92	.05	23.22	21.4%
FP	.43	.40		8.8%	41.4		76.3 Z	63.1% .01
SC	2.63	3.60	N.S.	4.06	2.65	.01	-	-
GSR	. 59	1.18	N.S.	2.15	1.02	.01	-	-
RR	15.9	15.1		5.3	5.4	N.S.	- 3.6	2.0

COLD PRESSOR SCORES

Table 21



...........

Figure 26) done on the fifth day of testing we find the number of misclassi-

fied subjects reduced to one control and one patient. A review of these two misclassified subjects confirms the patient to be clearly a chronic schizophrenic with no signs of improvement. The case history of the control subject does re. veal some difficulties in gaining emotional maturity with one

severe psychiatric breakdown but currently he is functioning well. Obviously our measures contain enough error to readily permit this much failure in classification even if our basic variables were primary to schizophrenia which as yet is quite unconfirmed. It is to be expected that upon replication these combined best discrimination scores would inevitably regress somewhat in their diagnostic power.

As yet we have not had an opportunity to utilize the response amplitudes to standard pain stimuli as possible correction modulators for the conditional responses, but they are included in Table 22 as a basic part of the findings.

Stimulus Intensity		Skin Con	ductance			Finger Po	Pulse			
		itrol 11	Schizophrenics N=21			ntrol =13		phrenics =21		
ma	Base (umho)	Response (umho)	Base (umho)	Response (umho)	Base (mv)	Response (% Change)	Base (πv)	Response (% Change)		
2.5	2.85	. 53	4.25	.93	15.2	32.5	19.1	42.4		
3.5	2.71	74	4.41	1.02	16.5	34.3	21.8	49.1		
4.0	2.59	1.18	4.42	1.27	15.8	39.1	21.8	51.6		
4.5	2.62	1.37	4.44	1.35	17.2	36.8	19.8	52.3		

BASE LEVELS AND RESPONSES TO 4 PAIN STIMULI FOLLOWING THE EXTINCTION SESSION

Table 22

Other aspects of a battery for best discrimination between two groups should include: (1) an increase in the range of difficulty of the items so as to optimally test each subject regardless of his aptitude; (2) to optimize the test item combinations by the discriminant function; (3) to replicate on new and larger groups; and (4) to purify or subdivide the groups into more homogeneous categories. This last notion of subdivision is very important. There are usually several mechanisms by which an individual copes with his problems. Some of these mechanisms such as "passivity" and "aggressiveness" which might serve fairly well by themselves, in combination may elicit maximum retaliatory reaction from the environment and cause great distress. Such incompatible or conflictual mechanisms may exist at the psychological (behavioral), physiological, and biochemical levels. Our test profiles must take into consideration these various styles of adjustment.

Simple linear combinations suitable for only monotonic variables such as the linear discriminant function cannot do this. The general finding that samples of schizophrenic patients nearly always have a wider range than normal on nearly all tests strongly suggests that two or more mechanisms are involved in their disability. The first step usually made in the attempt to recognize this heterogeneity is to classify schizophrenics into two groups on the basis of some variable. The presence or absence of a blood serum factor (Frohman, et al., 1961) or nor-epinephrine-like response to stress (Funkenstein, et al., 1957; Ax, 1953) are examples. Since such variables can operate in combination with still quite unknown results, they need to be simultaneously recorded and utilized together. This multiple variable team approach is being attempted at The Lafayette Clinic. Although we had in common a substantial group of schizophrenic patients on whom we

can intercorrelate our variables, our control groups were not in common and thus our comparisons are incomplete.

h. Non-Schizophrenic Low Motivation Subjects.

In order to test our hypothesis that low aptitude for autonomic conditioning should have profound relationships to social maladjustment other than schizophrenia we attempted to test a sample of skid row habitues who have a life history of low social motivation. Only four of these were successfully recruited, demonstrated to be free from physical and psychotic pathology and who would come into the hospital for two weeks for the diagnostic workup and psychophysiological testing. The scores analyzed on these show very similar results to those found for the schizophrenic group. The conditioning scores were as low or lower than for schizophrenia and the unconditional response to the pain stimulus was lower for skin conductance but essentially normal for finger pulse. Base level for skin conductance was low, BP was high. There were many circumstances such as age, alcoholism, chronically poor diet, etc. that make these subjects unsatisfactory. These were the main reasons why more were not tested.

Instead we undertook a research program (with Department of Labor assistance) to study students in the vocational retraining schools most of whom were school dropouts and adults who have had a long history of low achievement. These subjects will be classified as to evidence of motivation and also compared to other groups comparable with regard to race, education, socio-economic origin, I.Q., personality variables, age, etc., but who differ markedly with regard to achievement and social motivation.

B. Physiological Concomitants of Psychological Differentiation.

The results of the conditioning experiment indicated there was relatively little autonomic discrimination between the three tones. The question was raised as to what subject characteristics might relate to the discrimination variable. Mr. Courter and Dr. Watttenmaker were graduate students in psychology at Wayne State University and also were research assistants in our laboratory. They designed this experiment (Courter, Wattenmaker and Ax, 1965) to relate the cognitive style of "field independency" with autonomic differentiation. Field independency was measured by a "closure flexibility test" a form of imbedded figures test, and a "verbal concept attainment test". Forty normal college students served as subjects and were grouped into relatively higher and lower field independency. The group having the greater field independency very significantly (p < .01) better discriminated the tones by their GSR responses. "This study demonstrates that the stimulus generalization gradient involves an interaction between the cognitive style of the organism and the impinging stimuli, not merely the quantitative physical characteristics of the stimuli". These findings further suggest that the field dependent person may have a functionally less well-differentiated autonomic nervous system.

More research will be required to describe the functional relationships between perceptual discrimination and autonomic differentiation and the role learning plays in both, and their interactions.

IV. Conclusions.

The desirability of utilizing the digital computer for processing psychophysiological data is more obvious than ever. This study has clarified somewhat the problems in doing so and the specifications required for a practicable system. The difficulties which we experienced were due to an underestimation of the magnitude of the task and an over-estimation of our engineering resources. The best approach now (1967) would appear to be the use of an on-line type of computer with integral A/D and D/A converters and sampling under computer program control. Both analog and digital tape storage should be provided as backup when the computer is not available during data acquisition or when more computing is required than can be done in real time or when much less computing is required than real time requires so as to enable the computer to use its full speed potential by tape speedup.

Signal conditioning, including automatic editing by pattern recognition and less exotic methods, should be done both by analog and digital methods at various stages of the signals' progress through the system. An optimum compromise between early on-line analog signal conditioning and later digital manipulation must be worked out so as to maximize signal/noise ratio under the constraints of engineering and apparatus costs, signal distortion (such as lags due to analog filtering), digital computer speed, computing costs and time available. The nature of the variable, the parameters desired from it, and the local situation with regard to engineering sophistication, apparatus, and funds available all enter the compromise equation.

Sampling rates and resolutions should be kept to a minimum required to provide the information desired since the cost of digital computing is

roughly proportional to the number of bits to be processed. Flexible sampling rates under computer program control can often save a great deal of computing time.

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The system must be easily calibrated by the regular operator of the acquisition system on a daily basis or more frequently if necessary. Ideally where small drifts cannot be avoided a calibration signal for the variable which it calibrates should be periodically updated (manually or automatically) and carried along with the signal and made available to the computer program which should be able to normalize the computed values to the standard calibration. Time code event mark and ID mark must be provided for both polygram and magnetic tape and a tape search system provided so as to locate any record, event, or time on the analog record. Ideally, these codes should be automatically converted to appropriate digital values so as to avoid human work and error. It might appear that the above recommendations are merely obvious good engineering practice. In the practical laboratory situation, however, numerous compromises must be made. We have found the above considerations to be essential minimal requirements that cannot be ignored.

Our computing programs have not been used enough to provide the experience necessary for any conclusions or recommendations beyond the rationale for their design. The response approach and correlations among parameters of responses matched for minimal variance in lag appear to be a useful and theoretically valid approach.

The findings that the parameters of autonomic conditioning and the epi-norepi-like physiologic response patterns have great diagnostic

power indicates the method is well worthy of further study and application to other groups of interest. While there is still much to be learned by the classical conditioning method of autonomic processes in humans, the instrumental method may prove even more fruitful. Classical conditioning with laboratory stimuli may fail to involve the basic motives sufficiently to tap the significant aspects of human life. Instrumental conditioning which makes the reinforcement contingent on the physiologic response, on the other hand, is more potent in getting involvement. It also appears to be a better fit with natural real-life learning. Accordingly, a next logical step in the development of physiological indices of stress tolerance, motivational aptitude and emotional development should involve instrumental conditioning of autonomic processes.

Finally an area of motivation as much in need of clarification as the aptitude for motivational learning is that of <u>current motivation</u>. All performance tasks including intelligence, personality and aptitude tests, as well as our own tests of motivational aptitude, are influenced by the <u>current motivation</u> as they are by the aptitude under test. It would be of great value to have an index of current motivation independent of the performance and of antecedent conditions such as instructions, deprivations, or promises. We have made this investigation our highest priority for our next study. During a standard tracking task which serves as the criterion of motivation the physiological parameters of arousal will be monitored during several intensities of positive (money and visual feedback) and negative (pain) reinforcement. Conflictual motives and anxiety will also be investigated to determine whether they have

characteristic physiological patterns which can be identified and removed from the physiological indices of the arousal related to the criterion performance. The characteristic physiological patterns of pleasant and unpleasant reinforcement will be a very interesting byproduct of this study.

These studies can be of value to NASA and the theory of human motivation by demonstrating and describing some of the relationships between physiological response and the motivation aspect of performance efficiency. To the extent that positive results are obtained, the prediction equations can indicate how indices of physiological response can be used to monitor the motivation being brought to bear on performance and learning.

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Table 2

VARIABLE NO.

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515	2006 2076 2073 2072 2073 2069

10BLK IS 047520206010

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Table 2, Contd.

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TIME	VARIABLE NO.	3
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519 521	2291 2311 2309 2289 2284 2296 2305 2292 2289 2300 2297 2315 2323 2310 2307 2318 2324 2311 2309 2341	2309 2277 2263 2281 2287 2271 2268 2288 2297 2288
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56 J 56 J	2064 2079 2092 2016 2066 2077 2096 2065 2034 2040 2079 2093 2106 2089 2080 2089 2104 2121 2131 2147	2061 2064 2034 2046 2063 2051 2045 2083 2101 2085 2165 2151 2139 2151 2165 2151 2142 2116 2111 2091
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5 H 3 5 H 5 5 H 7 5 H 7 6 H 1 6 H 3 6 H 3 7 H 3 6 H 3 7 H 3	$\begin{array}{ c c c c c c c c c c c c c c c c c c c$	$\begin{array}{c} 1276 & 1194 & 1181 & 1192 & 1210 & 1193 & 1186 & 1190 & 1148 & 1110 \\ 1133 & 1118 & 1110 & 1116 & 1114 & 1114 & 1114 & 1114 & 1190 \\ 1196 & 1085 & 1068 & 1084 & 1101 & 1078 & 1038 & 1045 & 1058 & 1041 \\ 1064 & 1055 & 1068 & 1084 & 1101 & 1078 & 1038 & 1045 & 1058 & 1041 \\ 1064 & 1056 & 1084 & 1089 & 1077 & 1056 & 1076 & 1094 & 1077 \\ 1143 & 1130 & 1122 & 1129 & 1138 & 1119 & 1110 & 1126 & 1146 & 1129 \\ 1257 & 1265 & 1246 & 1257 & 1275 & 1257 & 1242 & 1259 & 1278 & 1265 \\ 1318 & 1307 & 1297 & 1314 & 1332 & 1313 & 1374 & 1317 & 1334 & 1321 \\ 1325 & 1326 & 1226 & 1257 & 1257 & 1247 & 1259 & 1278 & 1265 \\ 1318 & 1307 & 1297 & 1314 & 1332 & 1313 & 1374 & 1317 & 1334 & 1321 \\ 1394 & 1348 & 1325 & 1336 & 1354 & 1378 & 1379 & 1368 & 1339 \\ 1208 & 1286 & 1277 & 1297 & 1299 & 1281 & 1271 & 1285 & 1394 & 1368 & 1339 \\ 1208 & 1286 & 1277 & 1297 & 1318 & 1376 & 1379 & 1361 & 1345 \\ 1314 & 1372 & 1285 & 1297 & 1318 & 1376 & 1374 & 1316 & 1345 & 1346 \\ 1428 & 1286 & 1277 & 1297 & 1318 & 1376 & 1341 & 1342 & 1364 \\ 1428 & 1286 & 1277 & 1297 & 1318 & 1376 & 1348 & 1342 & 1366 & 1342 \\ 1450 & 1455 & 1450 & 1457 & 1457 & 1458 & 1473 & 1356 & 1343 & 1345 \\ 1452 & 1339 & 1326 & 1339 & 1368 & 1354 & 1346 & 1361 & 1382 & 1368 \\ 1477 & 1415 & 1400 & 1412 & 1430 & 1415 & 1405 & 1418 & 1441 & 1429 \\ 1461 & 1450 & 1455 & 1450 & 1470 & 1453 & 1437 & 1457 & 1578 & 1555 \\ 1566 & 1572 & 1537 & 1549 & 1514 & 1527 & 1548 & 1577 & 1558 \\ 1569 & 1548 & 1547 & 1557 & 1590 & 1542 & 1577 & 1592 & 1614 & 1577 \\ 1674 & 1663 & 1651 & 1664 & 1667 & 1687 & 1687 & 1677 \\ 1674 & 1669 & 1697 & 1671 & 1693 & 1716 & 1609 & 1679 & 1688 & 1697 & 171 & 1718 \\ 1730 & 1716 & 1701 & 1713 & 1718 & 1708 & 1698 & 1699 & 1681 \\ 1750 & 1677 & 1671 & 1718 & 1708 & 1678 & 1669 & 1687 \\ 1671 & 1670 & 1671 & 1718 & 1708 & 1678 & 1669 & 1687 \\ 1671 & 1670 & 1671 & 1713 & 1718 & 1708 & 1698 & 1699 & 1681 \\ 1730 & 1716 & 1701 & 1713 & 1718 & 1708 & 1698 & 1699 & 1681 \\ 1750 & 1676 & 1677 & 1713 & 1718 & 1708 & 1698 & 1699 & 1681 \\ 1771 & 1670 & 1671 & 1713 & 1718 & 170$
5 H 3 5 H 5 5 H 7 5 H 7 6 H 1 8 H 1	$\begin{array}{ c c c c c c c c c c c c c c c c c c c$	$ \begin{array}{llllllllllllllllllllllllllllllllllll$
5 H 3 5 H 5 5 H 7 5 H 7 6 H 1 6 H 3 6 H 3 7 H 3 6 H 3 7 H 3	$\begin{array}{ c c c c c c c c c c c c c c c c c c c$	$\begin{array}{c} 1276 & 1194 & 1181 & 1192 & 1210 & 1193 & 1186 & 1190 & 1148 & 1110 \\ 1133 & 1118 & 1110 & 1116 & 1114 & 1114 & 1114 & 1114 & 1190 \\ 1196 & 1085 & 1068 & 1084 & 1101 & 1078 & 1038 & 1045 & 1058 & 1041 \\ 1064 & 1056 & 1084 & 1074 & 1041 & 1078 & 1038 & 1045 & 1056 & 1041 \\ 1064 & 1056 & 1084 & 1089 & 1077 & 1056 & 1074 & 1094 & 1077 \\ 1143 & 1130 & 1122 & 1129 & 1138 & 1119 & 1110 & 1126 & 1146 & 1129 \\ 1257 & 1246 & 1218 & 1218 & 1230 & 1214 & 1202 & 1259 & 1278 & 1265 \\ 1318 & 1307 & 1297 & 1314 & 1332 & 1313 & 1374 & 1317 & 1334 & 1321 \\ 1326 & 1226 & 1276 & 1236 & 1356 & 1334 & 1323 & 1339 & 1361 & 1345 \\ 1344 & 1348 & 1325 & 1336 & 1354 & 1378 & 1339 & 1361 & 1345 \\ 1344 & 1248 & 1277 & 1297 & 1299 & 1281 & 1277 & 1296 & 1293 & 1261 \\ 1208 & 1286 & 1277 & 1297 & 1299 & 1281 & 1277 & 1294 & 1293 & 1261 \\ 1313 & 1302 & 1285 & 1297 & 1318 & 1376 & 1349 & 1368 & 1339 \\ 1208 & 1286 & 1277 & 1297 & 1318 & 1376 & 1349 & 1361 & 1345 \\ 1344 & 1348 & 1355 & 1339 & 1364 & 1373 & 1356 & 1339 & 1361 & 1345 \\ 1346 & 1286 & 1277 & 1297 & 1291 & 1271 & 1285 & 1305 & 1260 \\ 1298 & 1286 & 1277 & 1297 & 1318 & 1376 & 1294 & 1216 & 1345 & 1345 \\ 1357 & 1349 & 1356 & 1339 & 1364 & 1351 & 1346 & 1361 & 1382 & 1368 \\ 1477 & 1415 & 1400 & 1412 & 1430 & 1415 & 1405 & 1437 & 1354 \\ 1450 & 1455 & 1450 & 1450 & 1457 & 1548 & 1547 & 1555 \\ 1566 & 1557 & 1537 & 1549 & 1514 & 1527 & 1548 & 1577 & 1556 \\ 1569 & 1548 & 1547 & 1557 & 1590 & 1542 & 1574 & 1592 & 1614 & 1577 \\ 1674 & 1687 & 1677 & 1693 & 1716 & 1687 & 1688 & 1697 & 1771 \\ 1679 & 1647 & 1641 & 1649 & 1706 & 1647 & 1648 & 1647 & 171 & 1694 \\ 1771 & 1649 & 1641 & 1649 & 1706 & 1678 & 1689 & 1697 & 1671 \\ 1730 & 1716 & 1701 & 1713 & 1718 & 1708 & 1689 & 1671 & 1641 \\ 1750 & 1647 & 1641 & 1649 & 1706 & 1678 & 1699 & 1681 \\ 1771 & 1649 & 1671 & 1718 & 1708 & 1698 & 1699 & 1681 \\ 1771 & 1649 & 1671 & 1718 & 1708 & 1698 & 1699 & 1681 \\ 1730 & 1716 & 1701 & 1713 & 1718 & 1708 & 1698 & 1699 & 1681 \\ 1750 & 1641 & 1671 & 1718 & 1708 & 1688 & 1687 \\ 1671 & 1671 & 1671 & 1718 & 170$

Table 2, Contd.

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TIME						VAPIABLE	NO. 12							
515	1306	1 1 9 2 1 1 9 6 1	1393 1397	1303	1394 1392	1344 1394	1306	1392 1394	1390	1396	1101	1394	1390 1394	1304
519		1390 1393				1392 1390		1386 139					1386 1388	
523		1382 1388				1398 1387		1384 138					1391 1394	
527	1394	1397 1396	1393 1398	1 3 9 6	1399 1397	1402 1398	1403	1400 1400	1400	1476	1474	1474	1407 1405	1406
531	1410	1404 1410	1409 1414	1413	1414 1414	1418 1420		1420 1420			1476	1427	1426 1430	1432
535		1436 1443				1468 1469		1470 1470					1486 1490	
539		14HB 1494				1498 1499		1497 150					1500 1502	
543		1496 1501				1499 1498		1492 1491					1490 1490	
547 55)		1484 1488				1464 1482		1458 146					1456 1458	
555		1457 1454				1451 1450		1445 145					1446 1450	
559		1447 1448				1442 1440		1434 344					1434 1438	
563		1430 1438				1442 1442		1438 .144/					1441 1444	
567	1448	1438 1446	1438 1446			1444 1441		1438 1446					1442 1446	
571			1449 1446			1447 1438		1436 144					1443 1454	
575		1470 1482				1486 1481		1480 148/					1493 1502	
579		1504 1514				.1537 1534		1571 1517					1470 1468	
583	1466	1498 1462	1458 1467			1470 1471		1544 1559					1580 1588	
587 591		1594 1602				1618 1614		1614 1627					1621 1624	
595		1620 1627				1674 1620		1618 1622					1614 1620	
599		1612 1618				1611 1678		1606 1610					1602 1606	
603	1608	1602 1606	1602 1606			1602 1596		1590 1590	1590	1594			1589 1594	
607		1590 1594				1590 1586		1582 1587					1579 1586	
611		1582 1586				1580 1574		1574 1574					1566 1572	
615		1564 1566				1564 1557		1557 1560					1550 1558	
619	1556	1548 1550	1548 1548	1546	1549 1542	1548 1547	1548	1541 1544	1540	1547	1538	1547	1534 1540	17 94
623	1539	1533 1534	1530 1532	1528	1531 1524	1528 1522	1528	1522 1525	1521	1522	1518	1525	1517 1523	1516
627	1522	1516 1518	1518 1521			1521 1514		1514 1515					1506 1510	
631		1504 1506				1510 1502		1504 1506					1520 1506	
635		1507 1514				1530 1524		1577 1530	1526	1530	1576	1532	1524 1533	15?6
639.	1534	1529 1532	1530 1536	1534	1542 1534	1544 1538								
TIME.						VARIABLE	NO. 23							
515	518	905	910	920	910	908	926	915	913		92	913	901	
527	902	896	915	898	1478	1170	1 352	956	1556		21	910	1597	
539	902	908	910	902	908	915	913	930	918		0.8	911	913	
551	930	910	926 906	901 910	913 921	4C2 941	914 905	910 918	915 942		02	905	899	1
563	<u>709</u> 509	914	906	4061	910	913	915	924	934		74	2514	914	
587	921	\$12	908	974	905	908	900	917	912		24	924	917	
599	920	\$16	914	928	918	976	934	904	912		16	918	928	
611	501	913	918	906	907	921	908	908	914		34	963	1061	
623	54 R	944	945	954	1018	1000	914	921	930	9	13	915	914	
635	91 B	910	915	913	934	907								
t i mf						VARIABLE	ND. 27							
515	1804	180	1807	1806	1808	1807	1804	1808	1800		97	179A	1798	
527	1798	1 800	1802	1798	1795	1804	1798	1794	1794		94	1798	1895	
539	1810	1809	1810	1919	1810	1809	1808	1877	1805		96	1812	1810	
551	1810	1414	1812	1812	1810	1812	1812	1812	1812		12	1810	1812	
563	1809	1809	1809	1409	1804	1805	1806	1867	1809		<u>10</u> 66	1870	1878	
575	1801	1886	1812	1822	1834	1874	1848	1870	1868		69	1866	1964	
599	1864	1866	1864	1864	1864	1864	1860	1860	1862		67	1867	1959	
611	1857	1854	1848	1846	1849	1846	1843	1840	1842		36	1834	1836	
623	1833	1828	1826	1824	1826	1826	1827	1826	1826		28	1826	1822	
635	1824	1826	18 10	1430	1834	1832								

₽¶ LISTI	ING FUR	ID 04752020	6010	VA	x 1	HEART PERIO	D IN SECONDS
- TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURY
421.0	EE	0.90	0.	1110.0	EE	1.03	0.
427-0	BE 2	0.93	0. 0.	1110-1	HI	1.06	0.50
422.4	1 H	0.96	0.35	1111.2	BEP	1.05	0.
424-1	LU	0.92	-0.16	1111.9	EF	1.00	-0.14
426.2	HI	0.92	0.55	1115.6	8F	1.00	0.
426-9	LG	0.90	-0.26	1115.9	LO	0.97	-0.77
427.8	EEP	0.98	0.20	1117.0	EEP	1.06	0.
429.0	85	1.00	0.	1117.0	BEP	1.06	-0.
571.0	EE	1.04	0.	1118.0	HI	1.19	0.32
572.0	BEP	0.59	0.	1121.5	LO	0.94	-0.51
572.5	1.0	0.99	-0.51	1122.8	EEP	0.99	0.
5 .0	HI	1.00	0.51	1124.0	66	1.01	0.
5 6.5	LU	1.00	-0.59	1230.0	EE	0.99	0.
5.7.0	HI	1.00	0.69	1231.4	BEP	0.97	0.
577.8	EEP	1.02	0.	1231.9	LO	0.95	-0.31
577.8	BEP	1.02	0.	1233.0	HI	1.01	0.56
578.5	10	0.98	-0.35	1234.6	LO	0.97	-0.29
580.0	й	1.07	0.43	1237.0	HI	1.05	0.55
580.4	FF	1.03	-0.21	1237.2	EEP	1.03	0.
582.4	BR	1.05	0.	1239.0	BE	0.99	0.
583.6	EFP	1.05	0.	1304.0	ĒĒ	0.97	0.
585.0	BE	1.09		1305.4	BEP	0.91	0.
705.0	EE	0.48	0,	1300.2	LO	0.90	-0.54
706.6	BEP	1.04	0.	1367.2	нI	0.97	0.39
707.0	н	1.05	0.66	1309.5	LO	0.92	-0.41
709.3	E.C.	2.48	-0.35	13/1.2	EEP	1.01	Q.
710.3	ER	1.04	0.11	1371.2	BEP	1.01	0.
712.4	EEP	1.13	υ.	1373.0	ні	1.07	0.55
712-4	BEP	1.03	0.	1375.5	LU	0.98	-0.48
715.9	8 E	1.04	0.	1377.0	нι	1.04	0.55
716.5	LC.	1.00	-0.80	1377.0	EEP	1.04	0.
718.0	нı	1.30	0.28	1378.0	BE	1.00	0.
718.0	FEP	1.05	Ο.	1434.0	EE	0.97	0.
719.0	ЪE	1.00	0.	1435.5	LO	0.93	-0.47
855.0	L.F	6.97	0.	1485.8	BEP	0.97	0.
856.4	BEP	1.03	0.	1437.0	ні	1.00	0.59
857.0	ні	1.03	0.57	1486+0	LO	0.92	-0.40
857.6	L L	0. YH	-0.15	1491.0	EEP	1.01	o.
859.0	нт	1.0:	0.43	1493.0	8E	1.04	0.
859.5	LU	0.98	-0.10	1035.0	EE	0.94	0.
862.2	EE ?	1.05	ა.	1635.3	нı	0.98	0.19
862.2	REP	1.05	ა.	1636.0	BEP	0.98	0.
864.0	нТ	1.22	0.31	1536.1	EF	C.95	-0.16
865.6	EF	1.00	-0.32	1640.5	BR	0.94	0.
867.6	НЪ	1.00	0 .	1641.8	FEP	1.09	Ο.
868.0	ні	1.09	J.76	1641.8	BEP	1.09	0.
0.868	f F P	1-09	۰ ا •	1642.0	HI	1.09	0.51
869.0	d E	1.05	е.	1643.5	LÜ	1.02	-0.63
\$77.0	E E	1.11	υ.	1645.0	HI	1.08	0.69
978.4	6EP	じょうと	1 .	1645.5	LO	1.06	-0.29
979-2	НI	0.99	0.42	1647.0	HI	1.09	0.40
981-4	16	0.64	-0.05	1647.d 1649.0	EEP BE	1.07 1.04	0.
984.2	E E P	1-00	· •		EE		с .
586.0	ВĘ	1.12	¢.	1704-0	CC	0.98	C.

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Table 3. Heart Period in Seconds.

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	C2C0010			SUMMARY NO			DINTS OF INTEREST
VARIABLE I P	ICANI PERIOD II			30:114.41 10	L		51141.5 (51 11111.025)
EFCCH 2	112						
	BEG EPUCH	572.0	END EPOCH	577.8		DURATION	5.8
	BEG AMP	0.99	AT TIME	572.0			
	ENC AMP	1.02	AT TIME	577.8			
	MAX AMP	1.06	AT TIME	575.0			
	MIN AMP	0.99	AT TIME	572.5			······································
	MEAN AMP	1.02	STAN DEV	0.03			
100.C F	PER CENT GOOD	DATA	0. PER CENT LU	DNG EDIT	0.	PERCENTSI	ORT EDIT
	INIT AMP	INCREMENT	DURATION	LOPE	CURV	LATENCY	PREC DRIFT
FIRST INTERVAL	0.99	-0.01	0.5	-0.01		0.	
RESPENSE 1	C.99	0.08	2.5	0.03	0.51	0.5	0.
RESPENSE 2	1.06	-0.07	1.5	-0.05	-0.59	3.0	.
RESPENSE 3	1.00	0.07	0.5	0.13	0.69	4.5	0.
			0 0	0 05		E A	
LASI INTERVAL	1.06	-0.04	0.8	-0.05		5.0	
LASI INTERVAL			0.8 EREST SUMMÄRY	-0.05	. ·	5.0	
		POINTS OF INT			5, 1964		IONING
SESSICN NO 04752		PUINTS OF INT MUTTLEY (CCN	ERÉST SUMMÄRY			SECONDCONDI	IONING DINTS OF INTEREST
SESSICN NO 04752 Variaele 1 - P	2C2CoO1C N.	PUINTS OF INT MUTTLEY (CCN	ERÉST SUMMÄRY	ESTED MARCH		SECONDCONDI	
SESSICN NO 04752 Variaele 1 - P	2020010 N. -Eart Period 1	PUINTS OF INT MUTTLEY (CCN	ERÉST SUMMÄRY	ESTED MARCH		SECONDCONDI	
SESSICN NO 04752 Variaele 1 - P	20200010 N. -EART PERIOD 1 132	POINTS OF INT MUTTLEY (CCN N SECONUS	EKĖST SUMMÄKY TROLJ ID O317 1	ESTED MARCH		SECOND CONDI	DINTS OF INTEREST
SESSICN NO 04752 Variaele 1 - P	EART PERIOD I 152 Beg Epich	POINTS OF INT MUTTLEY (CCN N SECONUS 577.8	ERÈST SUMMÄRY TROL) ID D317 1 END EPOCH	SUMMARY NO		SECOND CONDI	DINTS OF INTEREST
SESSICN NO 04752 Variaele 1 - P	EART PERIOD IN 152 Heg EPCCh Beg Amp	PUINTS OF INT MUTTLEY (CCN N SECONDS 577.8 1.02	ERÈST SUMMÄRY TROLJ ID D317 1 END EPOCH AT TIME	583.6 577.8 580.0		SECOND CONDI	DINTS OF INTEREST
SESSICN NO 04752 Variaele 1 - P	EART PERIOD IN 152 BEG EPCCH BEG AMP END AMP	PUINTS OF INT MUTTLEY (CCN N SECONDS 577.8 1.02 1.05 1.07 C.98	EKĖST SUMMÄKY TROL) IG O317 1 END EPOCH AT TIME AT TIME AT TIME AT TIME	583.6 577.8 583.6 577.8 583.6 580.0 578.5		SECOND CONDI	DINTS OF INTEREST
SESSICN NO 04752 Variaele i f	20200010 N. -EART PERTUD II 152 BEG EPCCH BEG AMP END AMP MAX AMP	POINTS OF INT MUTTLEY (CCN N SECONDS 577.8 1.02 1.05 1.07	EKĖST SUMMÄKY TROLJ IO 0317 1 END EPOCH AT TIME AT TIME AT TIME	583.6 577.8 580.0		SECOND CONDI	DINTS OF INTEREST
SESSICN NO 34752 Variaele i n Efich 3	EART PERIOD I 152 HEG EPCCH BEG AMP END AMP MAX AMP MIN AMP	PUINTS OF INT MUTTLEY (CCN N SECONUS 577.8 1.02 1.05 1.07 C.98 1.04	EKĖST SUMMÄKY TROL) IG O317 1 END EPOCH AT TIME AT TIME AT TIME AT TIME	583.6 577.8 583.6 577.8 583.6 580.0 578.5 0.03	1	SECOND CONDI	DINTS OF INTEREST
SESSICN NO 04752 Váriáele 1 n Efich 3	20200010 N. -EART PERTUD I 152 BEG EPCCH BEG AMP END AMP MAX AMP MIN AMP PEAN AMP PER CENT GOOD	POINTS OF INT MUTTLEY (CCN N SECONDS 577.8 1.02 1.05 1.07 C.98 1.04 DATA	EKĖST SUMMÄKY TROLJ ID 0317 1 END EPOCH AT TIME AT TIME AT TIME AT TIME STAN DEV O. PER CENT LO	SUMMARY NO 583.6 577.8 583.6 580.0 578.5 0.03 DNG EDIT	0.	SECOND CONDIN 5 Pr DURATION PER CENT SI	DINTS OF INTEREST
SESSICN NO 04757 VARIAELE I F EFLCF 3 ICG.C /	ZCZCODIC N. EART PERIOD I ISZ BEG EPCCH BEG AMP MAX AMP MIN AMP MIN AMP PER CENT GOOD INIT AMP	POINTS OF INT MUTTLEY (CCN N SECONUS 577.8 1.02 1.05 1.07 C.98 1.04 DATA INCREMENT	EKĖST SUMMÄKY TROLJ IO 0317 1 END EPOCH AT TIMĖ AT TIMĖ AT TIMĖ STAN DEV O. PER CENT LO DURATION	583.6 577.8 583.6 577.8 583.6 580.0 578.5 0.03 DNG EDIT	1	SECOND CONDIN 5 Pr DURATION	DINTS OF INTEREST
EFLCH 3 FIRST INTERVAL	20200010 N. -EART PERIOD 1 152 BEG EPCCH BEG AMP END AMP MAX AMP MIN AMP PER CENT GOOD INIT AMP 1.02	PUINTS OF INT MUTTLEY (CCN N SECONDS 577.8 1.02 1.05 1.07 C.98 1.04 DATA INCREMENT -0.04	EKEST SUMMÄKY TROL) ID 0317 1 END EPOCH AT TIME AT TIME AT TIME AT TIME STAN DEV O. PEK CENT LO DURATION 0.7	583.6 577.8 583.6 577.8 583.6 580.0 578.5 0.03 DNG EDIT SLOPE -0.06	1 0. CUR V	DURATION	DINTS OF INTEREST
SESSICN NO 04757 VARIAELE I F EFLCF 3 ICG.C /	ZCZCODIC N. EART PERIOD I ISZ BEG EPCCH BEG AMP MAX AMP MIN AMP MIN AMP PER CENT GOOD INIT AMP	POINTS OF INT MUTTLEY (CCN N SECONUS 577.8 1.02 1.05 1.07 C.98 1.04 DATA INCREMENT	EKĖST SUMMÄKY TROLJ IO 0317 1 END EPOCH AT TIMĖ AT TIMĖ AT TIMĖ STAN DEV O. PER CENT LO DURATION	583.6 577.8 583.6 577.8 583.6 580.0 578.5 0.03 DNG EDIT	0.	SECOND CONDIN 5 Pr DURATION PER CENT SI	DINTS OF INTEREST

Table 4. Heart Period in Seconds - 6 Points of Interest.

PT LIST	ING FOR	ID 0475202	06010	V A	R 3	FINGER PUL	SE IN PERCEN	IT FULL RAN	GE		PAGE 4
TIME	TYPŁ	AMPL	CURV	T I ME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV
421.0	FE	6.45	۲.	1122.0	EEP	3.49	0.	1775.8	BEP	9.05	0.
422.0	BEP	6.10	ũ.	1124.0	BE	3.33	0.	1781.5	EEP	4.22	0.
423.1	ні	6.02	C•44	1230.0	E£	5.60	0.	1783.0	8E	3.57	0.
427.8	FEP	5.47	0.	1231.2	LO	5.32	-0.05	1918.0	EF	8.63	0.
429.0	BE	4.58	0.	1231.4	BEb	5.47	0 .	1919.0	BEP	7.92	0.
571.0	EE	8.60	0.	1233.0	ER	5.93	0.36	1919.7	LO	7.62	-0.41
572.0	BEP	8.73	С.	1237.2	EEP	5.72	0.	1920.7	нι	8.09	.0.26
574.8	HI	9.09	C.35	1237.4	8F	5.88	0.	1920.9	ЗSE	7.95	0.
577.8	EEP	7.05	υ.	1239.0	RE	5.30	θ.	1923.0	ESE	7.80	0.
577.8	BEP	7.65	0.	1304.0	Eξ	7.71	Û.	1924.8	EEP	6.52	0.
583.6	FEP	4.24	0.	1365.4	вер	7.05	0.	1924.8	BEP	6.52	0.
585.0	RE	3.32	0.	1366.0	LO	0.57	-0.48	1930.6	EEP	3.95	0.
705.0	£E	5.51	0.	1365.2	н	6.90	0.52	1932.0	ВE	3.31	0.
706.4	HI	6.40	0.45	1371.2	É E P	5.40	0.	2068.0	EE	6.81	0.
706.6	HEP	6.25	0.	1371.2	BEP	5.40	0.	2069.0	BEP	6.66	0.
712.4	FEP	5.14	0.	1377.0	EEP	4.07	υ.	2071.2	нI	7.40	0.26
712.4	I:E P	5.14	0.	1370.0	ßE	3.59	с.	2074.8	EEP	6.55	0.
718.0	FEP	3.67	С.	1434.Û	٤Ŀ	10.51	î.	2074.3	нЕР	6.55	0.
719.0	BE	3-43	0.	1485.2	LO	9.59	-0.54	2081.0	EEP	3.62	0.
855.0	ΕE	6-45	0.	1485.3	BEP	9.76	¢.	2082.0	BE	3.75	0.
856.4	PEP	6.87	0.	1487.4	нı	10.11	0.52	2188.0	EE	10.89	0.
859.7	н	7.37	0.47	1491.6	EEP	0.56	0.	2188.8	нI	11.23	0.58
862.2	E E P	0.35	ن .	1443.0	КE	8.19	0.	2139.6	360	10.79	0.
862.2	КEР	6.15	0.	1635.0	ÉÉ	10.55	J.	2190.2	LO	10.09	-0.50
868.0	ee b	3.54	Ο.	1636.0	HEP	10.98	0.	2192.4	нI	10.69	0.48
869.0	BE	3.24	٤.	1035.3	ні	11.09	0.45	2193.8	LÜ	10.02	-0.55
\$77.0	ŕE	7.11	0.	1637.7	LQ	10.53	-0.59	2195.2	HI	11.07	0.49
977.5	LO	6.80	-0.22	1639.1	нI	11.21	0.57	2195.4	EEP	10.20	0.
578.4	H F F	7.05	0.	1641.8	EEP	9.56	С.	2197.0	ŊΕ	7.14	0.
579.7	ы	7.36	0.50	1641.0	BEP	9.56	0.	2322.0	EE	10.49	0.
981.1	t a	6.50	-0.62	1047.0	EEP	3.78	0.	2323.8	BEP	9.96	0.
982.5	hI	7.27	0.49	1649.0	8E	3.28	0.	2323.9	LO	9.91	-0.34
984.2	EEP	6.44	Ο.	1769.Ū	` E£	9.95	0.	2326.1	HI	11.27	0.61
986.0	8 F	5.20	٤.	1759.7	LU	9.64	-0.21	2329.6	EEP	10.18	0.
1110.0	FE	9.Cü	Ο.	1770.0	BEP	9.75	. 0.	2329.6	BEP	10.18	0.
1111.2	BEP	4.05	0.	1771.1	HI	10.01	0.47	2335.6	EEP	4.92	0.
1117.0	EFP	6.32	Ο.	1775.0	FEP	9.05	Ο.	2337.0	BE	4.46	0.
1117.0	PFP	6.20	ů.								

Table 5. Finger Pulse in Percent Full Range - Var. 3

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PEINTS OF INTEREST SUMMARY

SESSIEN NO 041	520206010	NAME (CUN	IRUL) 10 0317	TËSTED MARCH	5, 1964	SECOND CONDITIO	INING
VARIALLE '3	FINGER PULSE I	N PERCENT FUL	L RANGE	SUMMARY NO	1	3 POIN	ITS OF INTEREST
EFELH 2	112						
	825 22008 825 202 265 202 845 202 847 847 847 847 847 847 847 847 847 847	572.0 8.73 7.65 9.69 7.05 0.45	END EPUCH AT TIME AT TIME AT TIME AT TIME STAN DEN	577.0		ΟυΡΑΤΙΩΝ	5.9
100.0	PLK ČENI GOGJ	1A1A	J. PER LENT I	LUNG EBIT	۰.	PER CENT SHAP	יד רסוד
FIRST INTERVAL Last interval	1011 AMH 2.13 5.05	18686MEN1 6.30 -1.45	004AT 10N 2.8 3.0	SECPF 0.13 (.48	CURV	EATENCY 0 0. 2.4	DALL USIEL

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PUINTS OF INTEREST SUMMARY

SESSIEN NO 647526266016	NAME (CC)	TROLI 10 0317	TESTED MARCH	5, 1964 SECUMO COMP	ETT INT NG
VARIABLE 3 FINGER PULSE	IN PERCENT FU	LL RANGE	SUMMARY NU	1 1	PHINTS OF INTEREST
EFLCF 3 152					
1355 EPOCH Deg Amp End Amp (Ax Amp)	577.8 7.65 4.24 7.65	FND EPUCH AT TIME AT TIME AT TIME	577.8 583.6	DURATION	5 . 4
MIN EMP Pean Amp	4 • 24	AT TIME STAN DE	583.5		
166.6 FER CENT GUL	D DATA	O. PER CENT	LUNG EDIT	O. PER CENT	SHORT FOIT
INIT AMF Firsi interval 7.65 Lasi interval 4.24	-3.40	DURATION 5.8 0.	SLOPE -0.59 0.	CURV LATENCY D. 5.8	PREC DRIFT

Table 6. Finger Pulse in Percent Full Range - 3 Points of Interest.

	PI LIST	ING FOR	10 0475202	06010	VA	R 12	SKIN POTEN	TIAL IN MILL	IVOLTS			PAGE 5
	TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV
	421.0	FE	-8.15	Э.	980.0	ßR	-7.78	0.	1649.0	BE	-10.99	0.
	422.0	BEP	-7.97	0.	982.0	ER	-9.85	0.30	1769.0	6 6	-1.41	0.
	474.4	BR	-8.53	0.	984.2	EEP	-9.95	0.	1770.0	BEP	-1.32	Ó.
	427.8	EEP	-10.99	J.	986.0	8E	-10.80	0.	1773.2	BR	-1.87	0.
	429.0	ВÉ	-11.18	0.	1110.0	EE	-2.50	0.	1775.8	EEP	-3.33	0.
	571.0	FE	-8.16	0.	1111.2	BEP	-2.50	0.	1775.8	BEP	-3.33	0.
	572.0	bFP	-7.78	0.	1113.4	BR	-2.60	с.	1781.6	EEP	-8.34	0.
F	572.4	E۴	-7.64	-0.62	1117.J	EEP	-6.01	0.	1783.0	в с	-9.71	
	574.4	88	-7.63	0. 1	1117.0	BEP	-6.01	0.	1918.0	EE	-2.64	0.
	575.8	ER	-9.85	0.60	1120.0	ER	-8.91	0.52	1919.0	BEP	-2.60	0.
	577.8	FEP	-10.14	0.	1122.0	BR	-9.38	0.	1920.8	BSE	-2.41	0.
	577.8	BEP	-10.14	0.	1122.0	FED	-10.42	с.	1921.8	8R	-3.10	0.
	578.4	BR	-10.19	0.	1124.0	BE	-11.09	0.	1922.6	ER	-3.65	0.50
	581.0	HI	-12.33	0.55	1230.0	ЕE	-3.15	0.	1923.0	ESE	-4.06	0.
	582.6	FF	-9.00	-0.62	1231.4	BEP	-2.96	Q.	1924.8	EEP	-3.93	0.
	583.6	EEP	-8.53	٥.	1237.0	BR	-4.06	0.	1924.8	3EP	-3.93	0.
	585.0	BÉ	-4.62	0.	1237.2	EEP	-4.25	0.	1925.4	9R	-4.11	0.
·	705.0	EE	-7 <u>.</u> ძყ	0.	1234.0	вE	-5.26	Ο.	1930.6	EEP	-7.41	0.
	706.2	۴ĸ	-8.44	0.32	1364.0	EE	-1.23	Ο.	1932.0	86	-8.20	0.
	706.6	REP	-8.49	C.	1365.4	BEP	~1.55	0.	2068.0	EE	-1.68	0.
	708.8	нк	-8.72	0.	1305.6	ER	1.87	0.29	2069.0	BEP	-1.96	0.
	712.4	EE P	-12.14	0.	1358.2	BR	-2.14	Ο.	2072.4	8R	-2.05	0.
	712.4	HEP	-12.14	0.	137).в	ER	-4.43	0.55	2074.8	EEP	-3.05	0.
	715.4	НΙ	-14.21	0.59	1371.2	EEP	-4.43	0.	2074.8	BEP	-3.05	0.
	716.0	EF	-13.10	-0.49	1371.2	BEP	-4.43	0.	2081.0	EFP	-7.97	Λ.
	718.0	HR	-13.29	0.	1373.0	BR	-4.76	0.	2082.0	ЪE	-8.72	. 0.
	718.0	₹ F P	-13.29	J.	1377.0	EEP	-9.10	0.	2198.0	EE	-3.05	0.
	719.0	Bč	-14.16	Û.	1378.0	8E	-9.76	· 0.	2189.6	BEP	-2.87	0.
	855.0	ЕC	-6.80	0.	1494.0	EE	-1.32	с.	2192.4	BR	-3.51	0.
	856.4	8E2	-0.52	ე.	1435.8	BEP	-1.00	0.	2193.8	ER	4.06	0.43
	855.0	BR	-6.85	٥.	1488.6	BR	-1.77	0.	2195.4	EEP	-4.11	0.
	867.2	FEP	-9.38	0 .	1491.6	EEP	-3.33	С.	2197.0	BE	-4.16	0.
	867.2	REP	-9.33	0.	1493.0	BE	-3.79	0.	2322.0	EE	0.31	0.
	864.6	нı	-11.33	- 0.53	1635.0	EE	-0 .7 8	0.	2323.8	BEP	0.35	0.
	866 . C	៤ថ	-10.33	-0.45	1636.0	BEP	-0.87	0.	2326.4	BR	-2.01	0.
	868.0	EEP	-11.14	0.	1638.8	BR	-1.14	0.	2329.6	EEP	-1.87	9.
	869.0	нe	-11.57	0.	1641.8	EEP	-3.15	0.	2329.6	BEP	-1.87	0.
	977.C	Eć	-ŝ.20	0.	1641.8	8 E P	-3.15	0.	2335.6	EEP	-7.22	0.
	978.4	865	-1.97	0.	1647.8	EEP	-9.10	C.	2337.0	BE	-7.59	ົ.

Table 7. Skin Potential in Millivolts - Var. 12.

PULNIS CH	INTEREST	SUMMARY
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SESSIEN NU 047	520206010	NÂME JÛN		TESTED MARCH	5, 1964	SECOND CONDIT	TONING	
VARIABLE 12	SKIN PUTENTIAL	IN MILLIVOLT	S	SUMMARY NO	1	5 PC	INTS OF INTERES	57
EFLCF 2	112							
	EEG EPUCH BEG AMP ENG AMP MAX AMP MIN AMP MEAN AMP	572.0 -7.78 -10.14 -7.64 -10.14 -8.05	END EPOCH AT TIME AT TIME AT TIME AT TIME AT TIME STAN DEN	577.8 572.0 577.8 572.4 577.8 1 24		DURATION	. 5 • 8	
100.0	PER CENT GOUD	UATA	O. PER CENT L	ONG EDIT	0.	PER CENT SH	ORT FOIT	
FIRSI INTERVAL Respinse i Last interval	INIT AMP -7.18 -1.83 -4.85	INCREMENT 0.14 -2.03 -0.28	DURATIJN 0.4 1.4 2.0	SLUPE 0.35 -1.45 -0.14	CURV 0.60	LATENCY 0. 2.4 3.8	PREC DRIFT	

POINTS OF INTEREST SUMMARY

SESSION NU 047520206010	NAME (CUNTRU	il) 10-0317	TESTED MARCH	5, 1964 5	SECOND CUMPET	TIONING
VARIABLE 12 SKIN PUTENTIA	L IN MELLIVEETS		SUMMARY NO	1	4 Pr	TNTS OF INTEREST
EFLCF 3 152						
BEG EPUCH Beg Amf End Amp Max Amp Min Amp Mean Amp 100.0 Pek Cent Gudl	577.6 -10.14 -8.53 -8.53 -12.33 -10.01	END EPOC AT TIM AT TIM AT TIM AT TIM AT TIM STAN D	E 577.8 E 583.6 E 583.6 E 583.6 E 581.0 EV 1.69	с.	DURATION PER CENT SI	5.8 HURT FOIT
INIT AMP FIRST INTERVAL -10.14 RESPONSE 1 -10.19 RESPONSE 2 -12.33 LAST INTERVAL -9.00	INCREMENT -0.05 -2.14 3.33 0.47	DURATION 0.6 2.6 1.6 1.0	SLOPE -0.08 -0.82 2.08 0.47	CURV 0.55 -0.62	L & TFNCY	PPFC DRIFT n. n.

Table 8. Skin Potential in Millivolts - 3 Points of Interest.

LIST	ING FÜR	ID 0475202	C6010	VA	₹ 23	MUSCLE TEN	SION IN MICR	OVOLTS			PAGE
TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CUR
421.0	EE	24.98	0.	864.0	EF	25.63	-0.50	1491.6	EEP	23.88	0.
422.0	REP	24.98	0.	658.J	BR	24.61	0.	1493.0	вE	23.44	0.
427.8	FEP	24.98	э.	668.0	EEP	24.61	0.	1635.0	EE	24.91	0.
429.0	8F	24.03	э.	859.0	RE	93.96	с.	1636.0	BEP	22.70	0.
571.0	F£	20.92	U.	977.0	££	24.91	0.	1641.0	вse	23.37	0.
572.0	BEP	24.63	U.	778.4	8EP	24.16	0.	1641.9	EEP	23.37	0.
577.0	PSF	24.32	J.	934.2	EEP	24.03	С.	1641.8	вEР	23.37	0.
577.8	EEP	24.40	0.	535.0	ВĒ	23.88	0.	1643.0	ESE	23.59	0.
577.8	BEP	24.4)	0.	1110.0	EE	22.48	О.	1647.8	EEP	24.61	Ο.
579.0	ESF	24.51	3 . .	1111.2	BEP	23.00	Q.	1648.0	BR	24.83	0.
587.6	EEP	20.00	D •	1115.0	вSE	24.25	<u>э</u> .	1649.0	ЧE	51.49	0.
584.0	BR	29.15	J.	1117.0	E E P	23.88	Λ.	1769.0	EE	23.14	0.
585.0	ВF	95.32	J.	1117.0	REP	23.88	Ο.	1770.0	вер	23.44	0.
705.0	<u>F</u> F	23.74	Ð.	1118.0	ESE	23.44	0.	1775.0	8 E	24.18	0.
706.6	8FP	25.34	з.	1122.8	EEP	24.25	с.	1775.8	EFP	24.18	0.
711.0	BR	25.13	J.	1123.0	BR	24.18	0.	1775.8	8 F P	24.18	0.
711.0	BSE	26.13		1124.0	BE	79.03	с.	2068.0	FE	25.05	0.
712.4	EEP	57.76	0.	1230.0	£Ε	24.32	ί.	2069.0	нЕр	25.34	0.
712.4	REP	59.16	υ.	1231.4	8EP	24.18	е .	2074.0	BSE	25.49	0.
713.0	ESF	70.44	õ.	1237.2	EEP	23.33	0.	2074.8	EEP	26.21	5.
713.0	ні	73.44	r.so	1238.0	BP	25.56	0.	2074.8	BEP	26.21	0.
715.0	£ F	27.21	-0.69	1239.0	BÉ	30.84	Ο.	2076.0	ESE	27.35	<u>.</u>
718.0	H K	25.17	0.	1304.0	EE	24.83	Ο.	2081.0	BR	27.49	0.
718.0	EEP	25.77	э.	1365.4	BEP	24.61	0.	2081.C	EEP	27.49	0.
719.0	BE	75.46	е.	1370.0	BSE	24.91	Û.	2032.0	8E	90.94	0.
855.0	FF	24.83	Э.	1371.2	EEP	23.90	0.	2158.0	EE	23.74	0.
856.4	BEP	23.56	Ú .	1371.2	ЧЕР	23.96	0.	2189.6	BEP	24.91	0.
861.0	BR	24.40	с.	1372.)	٤SE	23.29	C.	2195.4	EEP	25.34	0.
861.0	RSE	24.40	0.	1377.0	BR	23.29	0.	2197.0	ВE	.25.34	Ő.
862.2	FEP	29.60	Ċ.	1377.0	EEP	23.29	Ĉ.	2322.0	EE	23.14	ő.
862.2	8EP '	29.00	Ū.	1378.0	BE	75.09	0.	2323.8	BEP	23.51	0.
863.0	ESE	32.44	Ċ.	1434.0	EE	25.05	0 .	2328.0	BE	23.14	0.
863.0	H1	32.94	0.50	1405.0	BEP	23.37	ΰ.		0.	23014	

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Table 9. Muscle Tension in Microvolts.

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PUINTS LE INTEREST SUMMARY

NAME (CONTROL) ID C317 TESTED MARCH 5, 1964 SECOND CONDITIONING SESSIEN NE CARSELECCEUL 3 POINTS OF INTEREST SUMMARY NO 1 MUSCLE TENSION IN MICROVOLTS VARIALLE 25 EFECH 2 112 577.8 DURATION 5.8 CEG EFUCH 512.0 END EPOCH 572.0 LEG AMP 24.03 AT TIME LNC AMP 24.40 AT TIME 577.8 577.8 NAX AMP 24.40 AT TIME MIN AMP 24.03 AT TIME 572.0 NEAN AMP 24.25 STAN DEV 0.19 13.8 PER CENT SHORT FDIT 0. PER CENT LONG EDIT 80.2 FER CENT GUUD DATA SLOPE CURV LATENCY PREC DRIFT INTE AMP. INCREMENT DURATION FIRST INTERVAL 24.03 0.37 5.0 0.06 0. 5.9 0. LAST INTERVAL 24.+0 С. 0. PEINTS OF INTEREST SUMMARY SESSIEN NU U4/32L2LOLIU NAME (CENTRUE) ID 0317 TESTED MARCH 5, 1964 SECOND CONDITIONING MUSLEE TENSION IN MICKEVELTS 2 POINTS OF INTEREST VARIABLE 23 SUMMARY NO 1 EFULE 3 152 REG EPUCH 577.0 END EPUCH 583.6 DURATION 5.8 24.40 AT TIME 577.8 DEV ANN END AMP 28.00 AT TIME 583.6 NAX ANP 28.06 AT TIME 583.6 MIN AMP 24.40 577.8 AT TIME NEAN AMP 26.34 STAN DEV 2.43 0. PER CENT LONG EDIT 20.7 PER CENT SHORT EDIT 75.3 PER LENT GLUU DATA INCREMENT DURATION SLOPE CURV LATENCY PREC DRIFT INTI AMP FIRST INTERVAL 24.40 3.66 5.8 0.63 **C**. LAST INTERVAL 5.8 28.00 J. 0. 0.

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Table 10. Muscle Tension in Microvolts - 3 Points of Interest.

PI LIST	ING FUR	[1) 04752020	00110	VA	R 27	SKIN CONDU	CTANCE IN MI	CROMHOS			PAGE 7
TIME	TYPE	4/4PL	CURV	TIME	TYPE	AMPL	CURV	TIME	TYPE	AMPL	CURV
421.0	£٤	3.64	0.	1112.0	BSE	3.40	0.	1775.8	вЕР	3.06	0.
427.0	8EP	3.03	υ.	1114.0	ESE	3.34	0.	1777.0	8R	3.08	0.
426-0	яĸ	3.68	0 .	1114.0	LÜ	3.34	-0.48	1731.6	EEP	3.25	0.
427.8	FEP	3.73	Ο.	1117.0	EEP	3.41	с.	1783.0	BE	3.29	0.
429.0	вE	3.75	Ũ.	1117.0	BEP	3.41	Ο.	1918.0	FE	3.07	0.
571.0	FE	3.00	0.	1122.0	BSE	3.01	С.	1919.0	BEP	3.07	0.
572.0	HEP	3.61	0.	1122.3	EEP	3.61	Ο.	1920.0	BSE	3.07	0.
577.C	BR	3.62	0.	1124.0	ESE	3.60	0.	1923.0	ESF	3.07	0.
577.8	EEP	3.66	0.	1124.0	нE	3.60	Ο.	1924.8	FEP	3.11	0.
577.8	BEP	3.00	0.	1530-0	SE	3.25	0.	1924.8	BEP	3.11	0.
583.6	EEP	3.91	0.	1231.4	ьΕР	3.26	0.	1927.0	BR	3.11	0.
585.0	Br.	3.90	0.	1237.2	EEP	3.29	<u>o</u> .	1930.6	EEP	3.21	<u>0</u> .
705.0	۴F	3.57	0.	1239.0	ðЕ	3.30	с.	1932.0	BE	3.26	0.
704.6	dEP	3.50	Э.	1364.0	EE	3.16	С.	ZC68.0	£E	2.88	0.
711.0	BE	3 <u>.</u> 6ú	0.	1365.4	ЧЕР	3.16	0.	2059.0	BEP	2.89	0.
712.4	EEP	3.67	С.	1394.3	BR	3.20	Û.	2074.8	EEP	2.91	0.
712.4	нEР	3.01	ů .	1371.2	EEP	3.26	0.	2074.8	SEP	2.91	0.
714.0	EEP	3.43	0.	1371.2	BEP	3.26	0.	2076.0	5R	2.92	0.
719.0	BE	3.83	0.	1377.0	EEP	3.42	C.	2081.0	EEP	3.13	0.
855.0	FE	3.40	0.	1378.0	вE	3.43	Ο.	2082.0	8 E	3.21	0.
850.4	HEP	3.48	Ο.	1434.0	εe	3.07	0.	2188.0	EE	2.91	٥.
860.0	HR BR	3.51	0.	1485.d	8 F.P	3.09	Û.	2189.6	BEP	2.90	0.
862.2	EEN	3:59	0.	1491.6	EEP	3.14	G .	2192.0	нſ	2.98	0.03
862.2	KEP	3.04	0.	1493.0	ЗE	3.16	0 .	2192.0	5 S E	2.98	0.
868.0	E1: h	3.36	0.	1635.0	θE	3.03	0.	2194.0	ESE	2.90	0.
869.0	BE	3.00	0.	1630.0	BEP	3.02	С.	2195.4	EEP	2.89	Ū•
977. 0	E E	3.42	Ο.	1041.8	EEP	3.02	0.	2197.0	8E	2.91	0.
978.4	BEP	1.45	C.	1341.8	BEP	3.02	0.	2322.0	£Ε	2.82	0.
982.0	8 S E	3.00	с.	1044.0	ВR	3.08	0.	2323.8	6EP	2.78	0.
984.0	ESE	3.56	0.	1547.5	EEP	3.28	0.	2329.6	EEP	2.82	0.
984.2	EFP	1.56	С.	1549.0	вE	3.34	0.	2329.6	нер	2.82	0.
986.0	BE	3.57	υ.	1759.0	EE	3.03	0.	2331.0	BR	2.86	0.
1110.0	£έ	3.34	0.	1770.)	8 E P	3.04	с.	2335.6	666	3.07	0.
1111.2	REP	3.35	ũ.	1775.3	EEP	3.06	е.	2337.0	8E	3.09	0.
1112.0	ні .	3.43	0.25								

Table 11. Skin Conductance in Micromhos.

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		PUINTS OF INT	EREST SUMMARY				
SESSIEN NU U47520200010		NAME (CEN	TRUL) ID C317	TESTED MARCH	5, 1964 S	ECOND CONDIT	LONING
VFRIAELE 27	SKIN CUNDUCTAN	CE IN MICKOMH	ÚS	SUMMARY NO	1	3 PC	INTS OF INTEREST
EFLCH 2	112						
	BEG EPUCH BEG AMP ENU AMP MAX AMP MIN AMP MEAN AMP	572.C 3.61 3.66 3.66 3.61 3.03	END EPOC AT TIM AT TIM AT TIM AT TIM AT TIM STAN D	E 572.0 E 577.8 E 577.8 E 572.0		DURATION	5 . 8
100.0	PER CENT GOOD	DATA	0. PER ÜLNT	LONG EDIT	0.	PER CENT SH	ORT FOIT
FIRST INTERVAL Last interval	INIT AMP 61. ذ ۲. د ۲	INCREMENT C.01 C.05	DURATION 5.C 0.8	SLOPE 0.00 0.06	CURV	LATENCY 0 • 5 • 0	PREC DRIFT

PLINTS OF INTEREST SUMMARY

SESSION NO 047	520206010	NAME (CON	1KUL) ID 0317	TESTED MARCH	ዛ. 5. 1964	SECOND CONDIT	TONING
VARIABLE 27	SKIN CLINLUCIAN	NCE IN MICRUMH	ωs.	SUMMARY NO	0 1	1 PC	INTS OF INTEPEST
EFLLF 3	152						
	BEG EPUCH DIG AMP END AMP MAX AMP MIN AMP MEAN AMP	577.8 3.66 3.51 3.91 3.66 3.91	END EPOCH Al TIME AT TIME AT TIME AT TIME STAN DE	577.8 583.6 583.6 583.6 577.8		DURATION	5.8
100.0	PER CENT GOOD		O. PER CENT		0.	PER CENT SH	IORT EDIT
FIRST INTERVAL LAST INTERVAL	INIT AMP 3.00 3.91	INCREMENT C.25 C.	DURATION 5.8 0.	SLOPE 0.04 0.	CURV	LATFNCY 0. 5.8	PREC ORIFT

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Table 12. Skin Conductance in Micromhos - 3 Points of Interest.

Conversion of Data Logger Units to Physiological Values

The following formula is used to convert data logger units to physiological units: $Y = A + BX + CX^2 + DX^3$ where X = Data Logger Units (range 0 to 4095 for ± 10 volts)

and Y = Physiological Units.

The conversion values for each variable are as follows:

		A	В	С	D
Heart Period (seconds)	=	11063	+.000542299		
Finger Pulse Amplitude (% total range)	Ŧ	_2.03070	+.004868120		
Finger Skin Potential (MV)	=	48.5797	031005	0000057979	+.0000000013476
Integrated Muscle Potential (µV)	*	-66.842	+.132097	000039165	+.0000000048841
Smoothed GSR (µmhos)		-5.17890	+.004039820	+.000000449881	

Conversion of Voltage Changes as Recorded on the Polygraph to Changes in Physiological Units

By means of the following relationships it is possible to determine the amount of change in physiological variables from the fluctuations in voltage recorded on the polygraph.

Heart Period Change (10 mil. sec.). = .039 inch.

Finger Pulse Amplitude Change (.01% total range) = .00294 inch.

Finger Potential Change (.01 MV) = .00067 inch.

Integrated Muscle Potential Change $(.01 \ \mu V) = .0002$ inch.

Smoothed GSR (.01 μ mhos) = .00488 inch.