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performance testing and development of a micro-calorimeter based on Superconducting QUantum Interference Devices (SQUIDs) (1). Unlike other microdosimetric detectors that are used for investigating the energy distribution, this detector provides a direct measurement of energy deposition at the micrometer scale, that can be used to improve our understanding of biological effects in particle therapy application, radiation protection and environmental dosimetry. Temperature rises of less than 1µK are detectible and when combined with the low specific heat capacity of the absorber at cryogenic temperature, extremely high energy deposition sensitivity of approximately 0.4 eV can be achieved (2).

The detector consists of 3 layers: a tissue equivalent (TE) absorber, a superconducting absorber and a silicon substrate. Ideally all energy would be absorbed in the TE absorber and heat rise in the superconducting layer would arise due to heat conduction from the TE layer. However, in practice direct particle absorption occurs in all 3 layers and must be corrected for.

To investigate the thermal behavior within the detector, and quantify any possible correction, particle tracks were simulated employing Geant4 (v9.6) Monte Carlo simulations. The track information was then passed to the COMSOL Multiphysics (Finite Element Method) software. The 3D heat transfer within each layer was then evaluated in a timedependent model. For a statistically reliable outcome, the simulations had to be repeated for a large number of particles. An automated system has been developed that couples Geant4 Monte Carlo output to COMSOL for determining the expected distribution of proton tracks and their thermal contribution within the detector.

Preliminary results of a 3.8 MeV proton beam showed that the detector reaches the equilibrium state after 8 ns. It is estimated that 20% of the temperature rise in the superconducting absorber is due to heat conduction from the adjacent absorber which needs to be corrected for. The simulations were repeated for proton beams with energies of 2, 10, 62 and 230 MeV.

Keywords: micro-dosimetry, Monte Carlo simulations and micro-calorimeter

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Assessment tool to quantify and visualize treatment plan robustness regarding patient setup

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Purpose: Nowadays, during the evaluation process of patient treatment plans in radiotherapy, the plan robustness is typically not taken into account. This evaluation of treatment plans can be improved if a user friendly and efficient tool to assess the robustness of the treatment plan is provided. Thus, the aim of this work is to develop tools and methods to quantify and visualize the robustness for treatment plans including random and systematic patient setup uncertainties.

Materials and Methods: A setup error phase-space including systematic and random setup errors for translation and rotation is explored to determine the treatment plan robustness. For this purpose a robustness-map is created based on user-defined criteria defining the robustness for the treatment plan considered. These criteria subdivide the robustness-map for the setup error phase-space into a region compatible with these criteria and into another one that is not. Several different approaches were implemented to

quantify the plan robustness. One approach transforms the optimized dose distribution relatively to the patient geometry and, thus, dosimetric parameters or DVHs can be quickly estimated, but are limited with respect to accuracy. Hence, approaches using further dose calculations for the setup error phase space are needed to achieve reliable conclusions of the robustness. For this purpose, additional dose calculations using a different resolution of the setup error phase-space are performed guided by the robustnessmap achieved using the dose-transformation approach. The intermediate dose distributions are determined by nearest neighbor or triangular interpolation.

Results: A graphical user interface based on QT version 5.3.1 was developed to calculate and visualize robustness-maps. These robustness-maps allow treatment plan evaluation by analyzing the corresponding dose-differences and DVHs. Additionally, correlations of all quantities can be displayed such that the user is able to efficiently view the data by scrolling through the setup error phase-space. The creation of robustness-maps is useful to assess and compare the robustness of different treatment plans and was successfully applied to plans covering different tumor-sites. For the cases investigated in this work, differences in DVH parameters using the different approaches are within 5%.

Conclusions: The developed tool for visualization and analysis of robustness-maps is an easy and efficient way to compare the robustness of treatment plans. Moreover, clinical tolerance and action levels for patient setup can be determined in order to keep specified dosimetric parameters within a certain limit. This work was supported by Varian Medical Systems.

Keywords: treatment planning, plan robustness, patient setup

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Treatment of moving targets with active scanning carbon ion beams

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Purpose: In this paper we report the preliminary results of clinical use of organ motion mitigation strategies in the treatment of moving target with active scanned carbon ion beams.

Material and methods: Since September 2014 25 patients with tumors located in the upper abdomen and chest were treated with active scanned carbon ion beams.

Patients were affected by pancreatic adenocarcinoma, HCC, biliary tract cancers and sarcoma of the spine retroperitoneum and heart. Tight thermoplastic mask was selected as the optimal abdominal compression device. 4D CT scan with retrospective reconstruction, with phase signal obtained with Anzai system (Anzai Medical CO., LTD), was employed for planning. Automatic assignment of raw data to respiratory phases was checked and, if necessary, modified by the medical physicist. Planning was performed using end expiration phase. Planning CT scan were visually checked for motion artifacts. Contouring was performed on end expiration phase and on the adjacent 30% expiration and 30% inspiration phases. Beam entrance was selected in order to avoid the bowel in the entrance channel. The lung diaphragm interface was contoured in the different respiratory phases and beam angles were chosen to avoid passing tangential to the lung diaphragm ITV. IMPT was used for plan optimization. Plans were recalculated in adjacent phases and if DVHs were degraded in an unacceptable way they were modified iteratively. Weekly verification 4D CT scans were performed

and, if needed, a new plan was re-optimized adaptively. Set up was verified with gated orthogonal X rays and non-gated cone beam CT in treatment room. Threshold for gate-on signal was initially set at 10% pressure signal dynamic and qualitatively adjusted in an asymmetric way according to results of plan recalculation in 30% expiration and inspiration. Gating signal was fed to the accelerator to enable beam delivery. Each slice was re-scanned 5 times to smear out possible interplay effects. Acute and early toxicity was scored according to CTCAE 4.0 scale.

Results: GTV and diaphragm excursion between end expiration and adjacent 30% phases was reduced to less than 5 mm. GTV (D95%) and critical OAR (D1%) DVH in 30% inspiration and expiration phases showed on average minimal (less than 3%) differences as compared to planning end expiration plan. Toxicity was minimal with no G3 event; 15% acute G2 and 10% G2 toxicity at 3 months was observed.

Median follow up was rather short (3 months) nevertheless in 23 patients the dose limiting OAR was either stomach or small bowel or esophagus, therefore early toxicity data are informative.

Conclusion: Active scanning with carbon ion beams for the treatment of moving target using abdominal compression, 4D simulation, robust planning gating and rescanning is feasible and safe. Longer follow up is needed to evaluate oncological outcome

Keywords: organ motion, active scanning

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Carbon ion radiotherapy: do we understand each other? How to compare differentt RBE-weighted dose systems in the clinical setting.

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In carbon ion radiotherapy (CIRT), mainly two calculation models are adopted to define relative biological effectiveness (RBE)-weighted doses (DRBE): the Japanese Kanai model and the Local Effect Model (LEM). Taken the Japanese longest-term clinical data as a reference, the use of a different RBE model, with no correction for the Gy (RBE) scale, leads to deviations in target absorbed dose (Dabs) with a potentially significant impact on tumor control probability. In this study we validate a conversion method linking the two DRBE systems, confirming DRBE prescription dose values adopted in our LEM-based protocols.

The NIRS beamline was simulated with a Monte Carlo (MC) code, according to design information about elements position, size and composition. Validation went through comparison between simulated and measured pristine and Spread Out Bragg Peaks, ridge filter based, in water. CT scan, structure set, plan and dose files of 10 treatment fields delivered at NIRS were exported in DICOM format, for prostate (3.6 Gy (RBE)NIRS per 16 fractions), Head & Neck (4 Gy (RBE)_{NIRS} per 16 fractions) and pancreas (4.6 Gy (RBE)_{NIRS} per 12 fractions) patients. Patient specific passive system geometries (range shifter, MLC, compensator, collimator) were implemented, for each field, to simulate delivered Dabs distributions. The MC code was then interfaced with LEM to calculate D_{RBE} resulting from the application of a different RBE model to NIRS physical dose. MC and TPS calculated Dabs and $\mathsf{D}_{\mathsf{RBE}}$ were compared in terms of dose profiles and target median dose. Patient CT and structure sets were also imported in a LEM-based commercial TPS where plans were optimized prescribing the non-converted and converted $\mathsf{D}_{\text{\tiny RBE}}$ values, respectively.

The agreement between MC and measured depth dose profiles in water, in terms of particle range, peak to plateau ratio and spread out profile shape, demonstrated beamline model accuracy. Patient dose distributions were correctly reproduced by MC in the target region, with an overall target median dose difference < 2%. MC median D_{RBE} resulted 16% higher than NIRS reference, for the lower prostate dose

level, 10% for head and neck and 4.5% for pancreas, in agreement with respective LEM-based prescription doses, adopted in our protocols. Deviations are expected to be close to zero around a prescription D_{RBE} = 5 Gy (RBE). Aside from unavoidable differences in dose profile shape, severe target under-dosage was shown in LEM-based optimized plans, when uncorrected D_{RBE} were prescribed.

The delivery of a voxel by voxel iso-effective plan, if different RBE models are employed, is not feasible; it is however possible to minimize differences in dose deposited in the target. Dose prescription is a clinical task which ultimately depends only on the radiation oncologist clinical decision; in this study we made an attempt to avoid systematic errors which could potentially compromise tumor control.

Keywords: Relative Biological Effectiveness, carbon ion radiotherapy, Local Effect Model

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Experimental study of Radiation induced DNA damage by internal Auger electron cascade compared to external yrays

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Purpose: The aim of this study is to compare the radiation induced DNA damage done by internal Auger-electron cascades with external exposures of sparsely ionizing radiation such as y-rays.

Background: Auger emitters decay by internal conversion (IC) or electron capture (EC) producing a number of Auger cascade electrons. These electrons are so low in energy that their range in tissue is in the order of nm-µm. This means that if the decay happens nearby the DNA, the Auger cascade electrons can produce a cluster of complex DNA damage. These clusters of DNA damage are much harder to repair and are therefore believed to be much more harmful to the cell than dispersed DNA damage, which are primarily produced by low LET radiation. Due to their short tissue range and the severe DNA damage produced, Auger emitters may be able to kill only the target cell while sparing non-targeted cells. This makes them а potential tool for radionuclide therapy(1,2,3,4).

Material/Methods: In order to compare the radiation effects by the Auger emitter to that of external γ-rays we need to be able to estimate the dose delivered. As Auger cascade electrons have a very short range the precise spatial distribution of the decays is of high importance.

We are currently working with two Auger emitters, Cs-131 and La-135. First experiments have been performed using HeLa cells, which were incubated with either Cs-131 or La-