Safety and efficacy of heparin-bonded surfaces in cardiopulmonary bypass

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he first article on heparin surface bonding was published in 1963 by Gott, Whiffen, and Datton.¹ At that time, the development of bloodexposed surfaces with improved thromboresistance was of prime interest. In those days, device occlusion during cardiopulmonary bypass (CPB) was a current problem. The presence of a shunt line that allows the arterial filter to be bypassed in most CPB circuits is still a testament to this major weakness of perfusion. Fortunately, in the early days the arterial filters tended to thrombose before the heat exchangers and oxygenators, and bypassing them usually salvaged the procedure. However, increasing awareness

of this problem led to the development of more thromboresistant arterial filters with a variety of heparin surface coatings. The success of these efforts opened the door for systematic application of heparin surface coatings for filter screens at various positions in the CPB circuit. Routine clinical use of heparin-coated components was thus established. The practice remained unrecognized for many years because CPB appeared to be extremely safe in conjunction with full systemic heparinization as defined by an activated coagulation time (ACT) of more than 480 seconds.

Use of heparin-coated equipment for perfusion with low or no systemic heparinization again goes back to Gott, who introduced the Gott shunt for bypassing blood during repair of aneurysms of the descending thoracic aorta. This approach, which was adopted by many surgeons, provided evidence that perfusion devices did not require full systemic heparinization if their design and surface properties were adequate. However, almost 30 years of step-by-step development² were necessary to get access to the tip-to-tip heparin-coated CPB circuit that allowed, first, partial and, later, total CPB³ with low systemic heparin levels similar to those used in vascular surgery (ACT > 180 seconds). Even though a number of studies have demonstrated reduced blood loss and transfusion requirements after CPB with heparin-coated equipment and low systemic heparinization,^{4,5} this issue remains the subject of controversy.

In parallel, many groups documented that heparin surface coating of perfusion equipment reduced the perfusion-induced inflammatory response.⁶ These findings may be less striking in the clinical setting with full systemic heparinization, because of the significant noise level resulting from cardiotomy suction⁷ and other ancillary equipment. However, increasing evidence shows that heparin-coated perfusion equipment is beneficial, despite full systemic heparinization. Wahba and colleagues⁸ have demonstrated significant reduction of transoxygenator/heat exchanger pressure gradients for various heparin-coated devices as compared with uncoated devices during routine cardiac surgery. These findings suggest that the pressures between the main pump and the oxygenator/heat exchanger structure often reach critical levels in current clinical practice in which uncoated perfusion equipment is used. This phenomenon usually is unnoticed because the arterial pressure is not usually measured anterior to the oxygenator/heat exchanger structure. Obviously, routine CPB is still far from perfect.

Once more, Øvrum and colleagues have provided an important piece of work in this setting. Their most recent study⁹ involves 1336 patients undergoing routine coronary bypass with either Duraflo II (Baxter Healthcare Corp, Bentley Laboratories Division, Irvine, Calif) or Carmeda BioActive Surface (CBAS; Medtronic Inc, Minneapolis, Minn) heparin-coated CPB equipment with low systemic hepa-

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Received for publication Oct 2, 2002; accepted for publication Oct 19, 2002.

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J Thorac Cardiovasc Surg 2003;125:S90-1

Originally published in J Thorac Cardiovasc Surg 2001;121:200-1.

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0022-5223/2003 \$30.00+0

doi:10.1067/mtc.2003.239

rinization (ACT > 250 seconds). The 2 heparin coatings studied have very different histories, are chemically different, and are bonded differently. Baseline patient parameters and outcomes look similar for the 2 patient groups analyzed. The patients with Duraflo II–coated CPB equipment required less systemic heparin to maintain the target ACT than did the patients with CBAS-coated CPB equipment. Interestingly enough, patients in the Duraflo II group also required less protamine for neutralization of circulating heparin than did patients in the CBAS group. The authors suggest that heparin leakage from the Duraflo II coating, which is more common than leakage from the CBAS coating, can explain this finding. However, if free heparin originating from the coating would have to be neutralized toto the patient is interesting to the parameters in the coating to the parameters in the parameters in the coating to the parameters in the parameters in the coating to the parameters in the parameters in the parameters in the coating to the parameters in the parameters in

gether with injected heparin, thus completing the total amount of circulating heparin necessary to reach a certain target ACT, one would expect to see no difference for protamine requirements between the 2 groups analyzed. Alternatively, a higher rate of antithrombin III adsorption onto the CBAS coating can explain higher requirements for both circulating heparin and then protamine as compared with the Duraflo II group.

Other mechanisms are involved as well, but this theoretical discussion should not divert our attention from the fact that Øvrum and colleagues⁹ have operated on a substantial number of patients (1336) who underwent routine coronary bypass grafting with low systemic heparinization and no oxygenator obstruction. Their achievements include 4.6 \pm 1.3 distal anastomoses per patient, at least 1 internal thoracic artery anastomosis in 99.3% of the patients, homologous transfusions in only 4.3% of the patients, and a hospital mortality of 0.3% (4/1336 patients)! If this was the standard of care on January 1, 2000, the rest of us doing CPB operations, as well as those involved in blood banking, are facing a major challenge.

Of course, one has to be aware of the disadvantages of

perfusion with low systemic heparinization despite the use of heparin-coated equipment (eg, potential for device occlusion, stroke) and the technical hints to avoid them.³ However, to give this approach a fair trial, one must also consider the disadvantages of full systemic heparinization (eg, bleeding, homologous transfusion, transfusion-related infection with regularly updated additional microorganisms). Hence, although the CPB philosophy selected for a specific patient (full versus low systemic heparinization) is a tradeoff, it becomes more and more apparent that, effectively, there is no free ride!

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