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# MR exponential image in ischemic stroke: A preliminary evaluation

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## KEYWORDS

Exponential;  
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**Abstract** *Background and purpose:* Magnetic resonance (MR) diffusion images, including both the diffusion-weighted image (DWI) and the apparent diffusion coefficient (ADC), allow detection of cerebral ischemic lesions within minutes of onset, and the contrast within the image is based on microscopic motion of the water. A third type of diffusion image can be created, “the exponential image”. Our goals were to evaluate the ability of exponential image in reflecting the changes in both DWI and ADC and whether it can replace these two sets of images in cerebral infarction patients.

*Patients and methods:* A total of 51 patients were enrolled in the study, 47 were included in the analysis, and four were excluded from the study. Conventional and DW MRI were performed in 47 patients. For each patient DWI, ADC maps, and exponential images were reviewed and the change in signal intensity of the lesion compared with the contralateral normal side was measured (rSI) as well as the changes in (rADC).

*Results:* There was a significant change in the rSI<sub>DW</sub> and rSI<sub>Exp</sub> in late subacute and chronic stages ( $p < .001$ ), however, rADC showed a significant decrease ( $p < .001$ ) in hyperacute and acute stages, followed by a significant increase ( $p < .001$ ) in the late subacute and chronic stages. rSI<sub>Exp</sub> was highly correlated with the change in the rADC values in different stages of infarction ( $r = .72, p < .001$ ). However, the changes in the rSI<sub>DW</sub> correlated less closely with the change in the rADC values ( $r = .35, (p < .05)$ ).

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*Conclusion:* Exponential image offers a simple, more accurate replacement for both sets (DWI and ADC), by combining the advantages of both sets.

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## 1. Introduction

Diffusion-weighted MRI (DWI) has shown increasing potential as a probe of tissue microstructure due to its sensitivity to the restricted diffusion caused by structural barriers that limit water mobility in vivo (1,2) as first described by Stejskal and Tanner (3).

In contrast to conventional MR imaging without diffusion weighting, DW imaging provides detection of lesions in the first hours after the onset of clinical symptoms (4).

DWI allows the discrimination between lesions with increased diffusion (due to vasogenic edema) and decreased diffusion (due to cytotoxic edema). The level of diffusion weighting is indicated by the  $b$ -value, a parameter that reflects the length and strength of the field gradients applied in the pulse sequence (1).

Because cytotoxic edema is thought to occur early in brain ischemia, DWI is highly sensitive in the early detection of brain infarctions (5,6). It provides important pathological–physiological information as well as the possible reversibility of tissue injury (7,8). Because “time is brain,” early diagnosis with early treatment is expected to improve outcome (9).

In acute cerebral ischemia, the area of restricted diffusion is identified as an area of signal increase against a hypointense background (9,10). The hyperintense appearance of acute infarcts on diffusion-weighted images results from a combination of abnormal diffusion and the intrinsic  $T_2$  properties which is difficult to determine on diffusion-weighted images alone. Small lesion size, brainstem lesions, and small cortical lesions on DWI performed within a few hours after stroke onset were associated with a particular risk of false-negative DWI-images (11–13).

In addition, infarcts can occasionally continue to appear hyperintense on DWI in the late subacute and chronic stages (i.e., when the increase in signal intensity due to restricted water diffusion is expected to begin to decrease) because of progressive  $T_2$  prolongation rather than a decrease in diffusion “ $T_2$  shine-through effect” (14).

The method that measures the rate of diffusion in living systems and not the characteristics of the  $T_2$  signal is referred to as the apparent diffusion coefficient (ADC). The ADC, a measure of the freedom of water diffusion, is believed to be low because of a shift of water, within hypoxic brain parenchyma, from the extracellular to the intracellular compartment where water diffusion is relatively restricted (15). Areas with a high diffusion will have a high ADC value and appear consequently hyperintense on the ADC maps (e.g., CSF) (9).

It is well accepted that ADC values decline rapidly after the onset of ischemia and subsequently increase and return to (pseudo)normal values, until it reaches supernormal values in a variable time course of about 17 days (16).

This technique (ADC) has drawbacks because it requires generation and interpretation of a set of ADC maps with the diffusion-weighted images. Another drawback is that these maps have different contrast characteristics from those of dif-

fusion-weighted images to which radiologists have become accustomed (17).

To remove the  $T_2$ -weighted contrast, the DW image can be divided by the echo-planar spin-echo  $T_2$ -weighted (or  $b = 0$  s/mm<sup>2</sup>) image to give an “exponential image” that combines the advantages of DW images and ADC maps (18).

The exponential images are a single set of MR images that show abnormal signal intensity because of restricted diffusion while negating the contribution of  $T_2$  signal intensity to DWI, and with high lesion conspicuity (19).

The aim of this study is to evaluate the ability of MR exponential diffusion-weighted images in diagnosing cerebral infarction, and whether it can replace the combination of the two sets of diffusion-weighted images and ADC maps.

## 2. Patients and methods

### 2.1. Selection of patients

This study was conducted on 51 patients. Inclusion criteria were: patients with a presumed diagnosis of infarct age that could be accurately determined on clinical ground, and were from less than 6 h to more than 2 weeks. All patients had no contraindications to MR imaging.

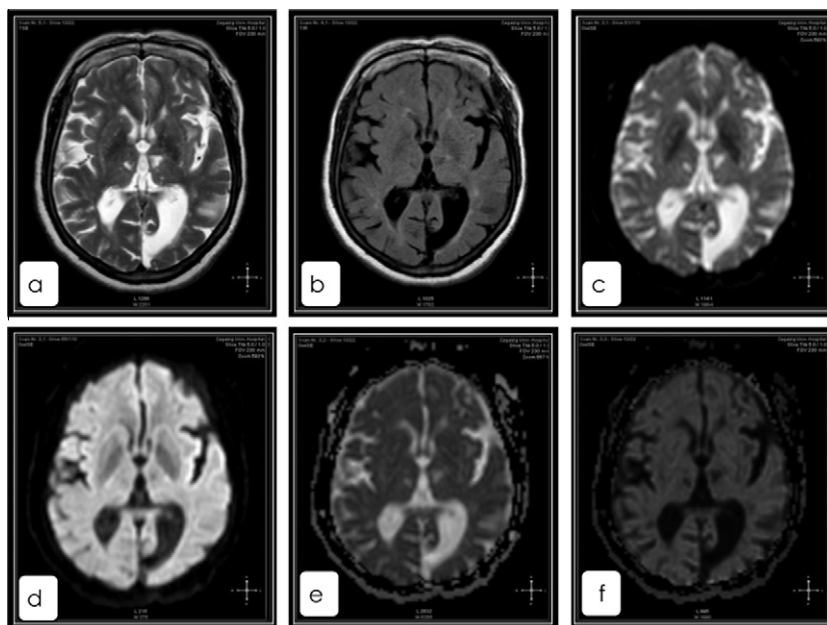
Exclusion criteria were: patients with a non-ischemic lesion that could have been responsible for the symptoms, severe hemorrhage, or patients with active seizures. These criteria yielded 47 patients out of the 51 patients enrolled in the study (31 males and 16 females), the mean age range was  $68 \pm 11$  years. A consent was taken from all patients. Four patients were excluded from the study, one patient had severe hemorrhagic infarction which interfered with image interpretation, two patients were uncertain about the time of the symptom onset, and one patient refused to complete the examination.

### 2.2. MRI

MRI was performed on a 1.5-T unit with (Philips Achieva System) with echo-planar capability. We performed the *standard MRI examination* as follows: axial  $T_1$  (TR148-97/TE2-15), axial  $T_2$  (TR4400-4800/TE110), axial flair (TR6000/TE120-TI2000). The imaging parameters were: matrix size was  $256 \times 128$ . Section thickness was 5 mm with a gap of 1 mm. The number of sections was set to include the whole brain (average, 22). DWI examination was acquired using a multisection, single-shot echo-planar imaging sequence, we used the same section thickness, interslice gap and number of sections as a standard MRI examination, with parameters of (TR 3100-3400/TE 98-99). For each slice, two diffusion weightings ( $b = 0$  and  $b = 1000$  mm<sup>2</sup>/s) were applied along the  $x$ ,  $y$ , and  $z$  axes, scanning time was 1 min 15 s. ADC maps (apparent diffusion coefficient) were automatically calculated by MRI machine software and included in the sequence of DW imaging. *Exponential images* were obtained

**Table 1** Shows relative signal intensity in DWI ( $rSI_{DWI}$ ), relative signal intensity in exponential images ( $rSI_{Exp}$ ), and relative ADC ( $rADC$ ) in different stages of infarction.

Stage of infarction	No. of patients	$rSI_{DWI} \ b = 1000$ (mean $\pm$ SD)	$rSI_{Exponential \ image}$ (mean $\pm$ SD)	$rADC_m$ (mean $\pm$ SD)
Hyperacute stage	13	$1.87 \pm 0.21$	$1.46 \pm 0.22$	$0.602 \pm 0.07$
Acute stage	11	$1.96 \pm 0.26$	$1.57 \pm 0.24$	$0.451 \pm 0.05$
Early subacute stage	8	$1.76 \pm 0.18$	$1.33 \pm 0.12$	$0.723 \pm 0.09$
Late subacute stage	6	$1.43 \pm 0.21$	$1.14 \pm 0.13$	$1.061 \pm 0.03$
Chronic stage	9	$0.96 \pm 0.18$	$0.62 \pm 0.27$	$2.198 \pm 0.07$

**Fig. 1** Chronic infarction after 3 months of symptoms. There are two small well-defined infarctions at both thalami displaying high signal intensity at T2WI (a), DWI- $b = 0$  (c) and low SI at FLAIR (b). The lesions display intermediate SI at DWI- $b = 1000$  (d) and high SI at ADC map (e). At exponential image (f) they display low signal intensity denoting chronic infarction.

automatically by dividing the DWI by the echo-planar spin-echo  $T_2$ -weighted (or  $b = 50 \text{ s/mm}^2$ ) image to remove the  $T_2$ -weighted contrast.

The regions of ischemic lesion on the DWI ( $b = 1000$ ), the exponential images, and on the ADC maps were analyzed by manually outlining the regions of interest (ROI) on the lesion and the corresponding normal contralateral tissue; then the relative SIs ( $rSI_{DWI}$  and  $rSI_{Exp}$ ) and the relative ADCs ( $rADC$ ) quotients of the lesion and control values were calculated.

### 2.3. Statistical analysis

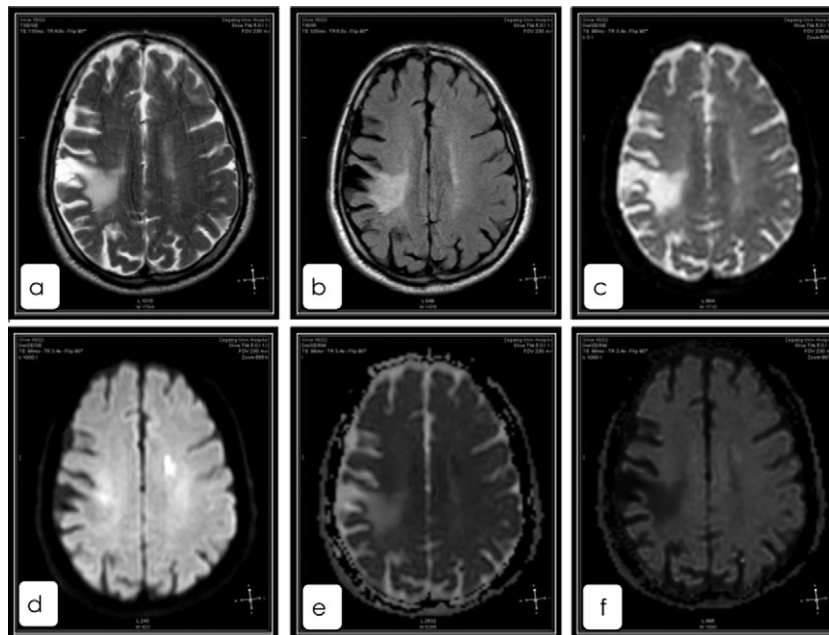
Statistical analysis was done using SPSS version 13. The mean and standard deviation were calculated for the rSIs and rADCs of each lesion. One-way analysis of variance (ANOVA test) for comparison between several means and LSD for least significance difference were done. The probability ( $p$  value) was considered non-significant when  $p > .05$ , significant when ( $p < 0.5$ ), and highly significant when  $p < .001$ . Finally, we correlated the mean change in signal intensity on both diffusion-weighted images and exponential images with the change in the ADC using Spearman rank correlations.

### 3. Results

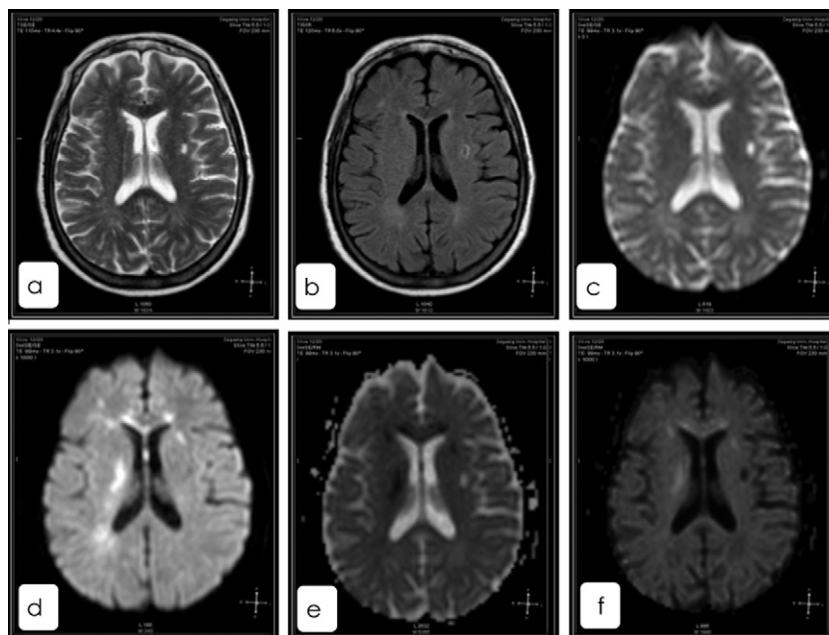
Fifty-one patients were enrolled in the study, and 47 were included in the analysis (31 males and 16 females), the mean age range was  $68 \pm 11$  years. Four patients did not meet the criteria of patient selection and were excluded from the study, one patient had severe hemorrhagic infarction which interfered with image interpretation, two patients were uncertain about the time of the symptom onset, and one patient refused to complete the examination. Based on clinical background and duration of symptom onset, thirteen patients had hyperacute infarcts (less than 6 h duration), eleven patients had acute infarcts (6–24 h), eight patients had early subacute infarcts (1–7 days), six patients had late subacute infarcts (less than 2 weeks duration), and nine patients had chronic infarcts (more than 2 weeks duration-up to 37 days).

In all patients, the changes in  $SI_{DWI}$  of the infarct (compared with those of normal tissue) were significantly higher ( $p < 0.001$ ) than in  $SI_{Exp}$  images.

The  $rSI_{DWI}$  (Table 1) showed a progressive increase from hyperacute infarcts ( $1.87 \pm 0.21$ ) (Fig. 3) to acute infarcts ( $1.96 \pm 0.26$ ) (Figs. 5, 6). In the early subacute stage, the  $rSI_{DWI}$  showed no significant decrease ( $p > 0.05$ ) ( $1.76 \pm$



**Fig. 2** Chronic infarction 6 months after symptoms. Axial T2WI (a), FLAIR (b) and DWI-b = 0 (c) show hyperintense area of infarction at the right posterior parietal region, and of intermediate signal intensity at DWI-b = 1000 (d) and high signal intensity at ADC map (e). At exponential image (f) the lesion displays low signal intensity denoting chronic infarction.

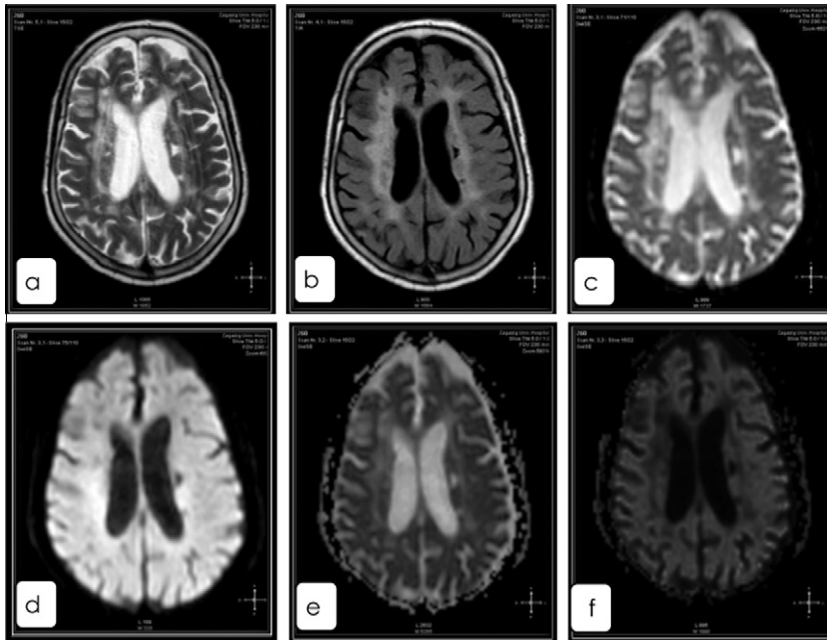


**Fig. 3** Multiple hyperacute right periventricular infarctions after 5 h of symptoms. The lesions cannot be detected at axial T2WI (a), FLAIR (b) and DWI-b = 0 (c) however at DWI-b = 1000 (d) they display marked hyperintensity, and low signal intensity at ADC map (e). The lesions display high signal intensity at exponential image (f) denoting hyperacute infarction. Another associated left periventricular chronic lacunar infarct which is of high SI at T2WI, FLAIR, DWI-b = 0 and ADC map, intermediate signal intensity at DWI-b = 1000 and low SI at exponential image denoting chronic infarction.

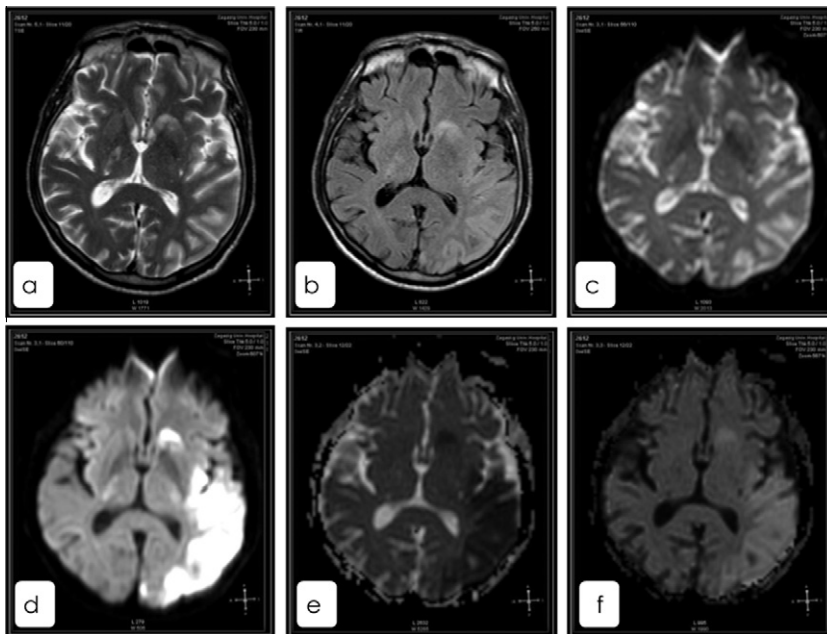
0.18); however in late subacute (Fig. 8) and chronic (Figs. 1, 2, 4) stages a significant progressive reduction ( $p < 0.001$ ) was seen in the  $rSI_{DWI}$  ( $1.43 \pm 0.21$  and  $0.96 \pm 0.18$ , respectively).

The mean  $rSI_{Exp}$  (Table 1) showed a progressive increase from hyperacute infarcts ( $1.46 \pm 0.22$ ) to acute infarcts (markedly hyperintense,  $1.57 \pm 0.24$ ), with no significant





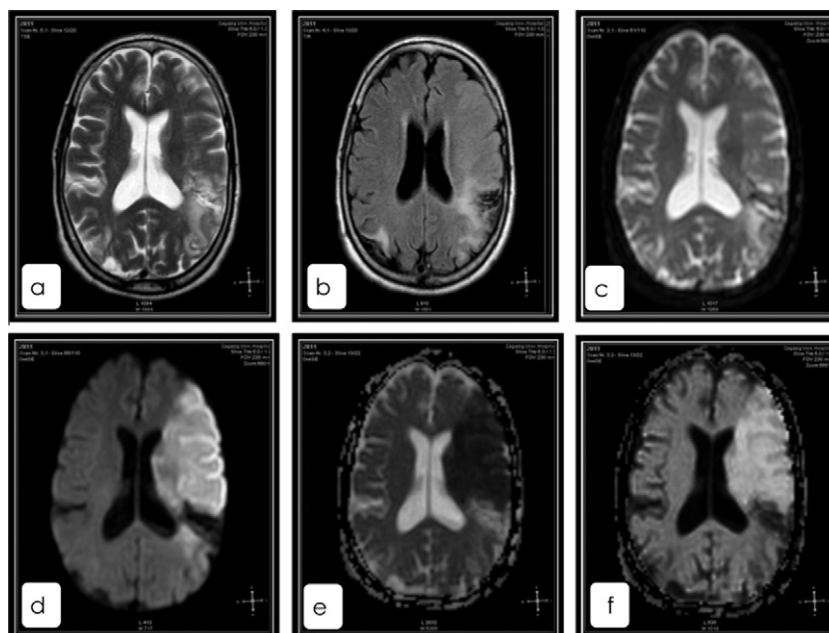
**Fig. 4**  $T_2$  “shine through” in subcortical arteriosclerotic encephalopathy patient show multiple small infarcts of high signal intensity seen at the periventricular regions displaying high SI at T2WI (a), FLAIR (b), DWI-b = 0 (c), DWI-b = 1000 (d) and ADC map (e) however it is of low SI at exponential image (f) denoting chronic infarcts. These findings are consistent with elevated diffusion secondary to microangiopathic change rather than acute infarction suggested by the DWI-images alone. Another solitary chronic left periventricular lacunar infarction of high SI at T2WI, DWI-b = 0 and ADC map and of low SI at FLAIR, DWI-b = 1000 and exponential images denoting chronic infarction.



**Fig. 5** Acute infarction after 8 h of symptoms at the left cortical parieto-occipital region. Axial T2WI (a), FLAIR (b) and DWI-b = 0 (c) show subtle increase in SI at the site of infarction. The lesion displays marked hyperintensity at DWI-b = 1000 (d) and low signal intensity at ADC map (e). At exponential image (f) it is of high signal intensity denoting acute infarction.

decrease ( $p > 0.05$ ) ( $1.33 \pm 0.12$ ) in the early subacute infarcts. Both the late subacute (iso-intense) and chronic stages (hypointense) showed a significant progressive ( $p < 0.001$ ) reduction in the mean  $rSI_{Exp}$  ( $1.14 \pm 0.13$  and  $0.62 \pm 0.27$ , respectively).

The mean  $rADC$  (Table 1) showed a progressive significant decrease ( $p < 0.001$ ) in hyperacute and acute stages ( $0.602 \pm 0.07$  and  $0.451 \pm 0.05$ , respectively), this was followed by gradual increase from  $0.723 \pm 0.09$  in the early subacute stage to a



**Fig. 6** Acute infarction after 7 h of symptoms at the left parietal region. Axial T2WI (a), FLAIR (b) and DWI-b = 0 (c) show subtle increase in SI at the left parietal region. The infarction is of marked hyperintensity at DWI-b = 1000 (d) and it is of low signal intensity at ADC map (e). At exponential image it is of high signal intensity denoting acute infarction. Another chronic infarction posterior to the acute one which is of high SI at T2WI, FLAIR, DWI-b = 0 and ADC and of low SI at DWI-b = 1000 and exponential image denoting chronic infarction.

**Table 2** Shows Spearman rank correlation coefficient of  $rSI_{DWI}$  and  $rADC$ , and  $rSI_{Exp}$  and  $rADC$  in 47 patients.

rSI	rADC	
	Correlation coefficient ( $r$ )	Probability value ( $p$ )
$rSI_{DWI}$	0.35	> 0.05
$rSI_{Exp}$	0.72	> 0.001

significant increase ( $p < 0.001$ ) reaching a pseudonormal level in the late subacute ( $1.061 \pm 0.03$ ), and a supernormal level in chronic stages ( $2.198 \pm 0.07$ ). The change in the  $rSI_{Exp}$  was highly correlated with the change in the  $rADC$  values in different stages of infarction ( $r = 0.72$ ,  $p < .001$ ) (Table 2). However, the changes in the  $rSI_{DWI}$  correlated less closely with the change in the  $rADC$  values ( $r = 0.35$ ,  $p < .05$ ) (Table 2).

#### 4. Discussion

The diagnosis of acute ischemic stroke by the use of conventional MR sequences is limited because of their relative insensitivity during the initial onset of neurologic deficit (20,21). Diffusion-weighted MR imaging has been shown to be an early marker for developing infarction (22–24) and rapidly becoming an integral part of the diagnostic workup in the acute stroke setting, as it is possible to identify severely ischemic brain regions within minutes to hours after stroke onset with a relatively high sensitivity and specificity (25–27).

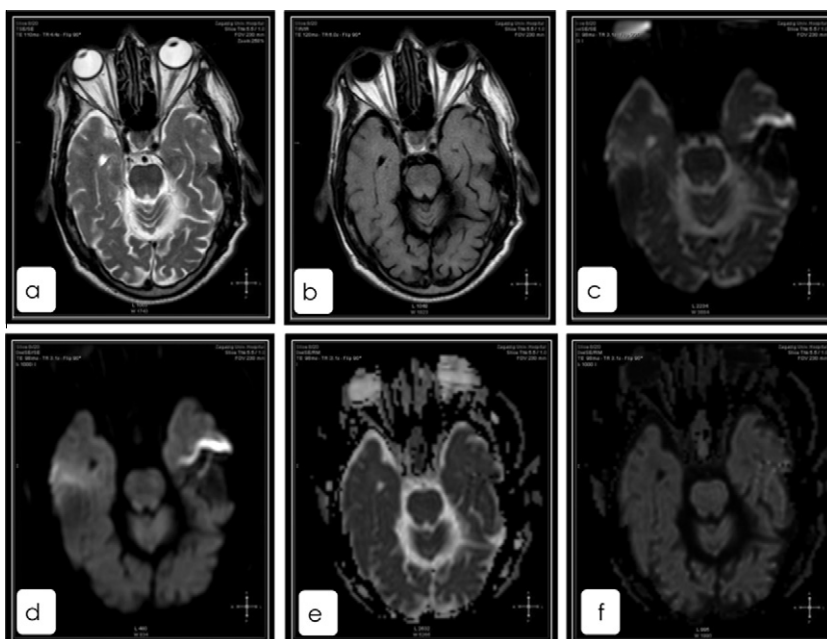
In human brain the ADC decreased rapidly as early as 30 min after vascular occlusion, and continues to decrease with peak signal reduction at 1–4 days (hyperacute and acute

stages). The reduction in ADC is mainly due to cytotoxic edema associated with decreased diffusion, so the lesion appears hypointense on ADC, hyperintense on DWI and less hyperintense on exponential images. The ADC returns to pseudonormal values after 1–2 weeks. This stage (subacute) is consistent with both cytotoxic edema (restricted diffusion) and vasogenic edema (increased diffusion); at this stage the lesion is mildly hyperintense on DWI due to water diffusibility and  $T_2$  component ( $T_2$  shine through) and iso-intense on ADC and exponential images. Subsequently, supranormal values of ADC are seen at chronic stage (more than 2 weeks), and it is attributed to increased extracellular water, tissue cavitation and gliosis, the lesion appears iso- to slight hypointense on DWI, hyperintense on ADC maps and hypointense on exponential images (28–30).

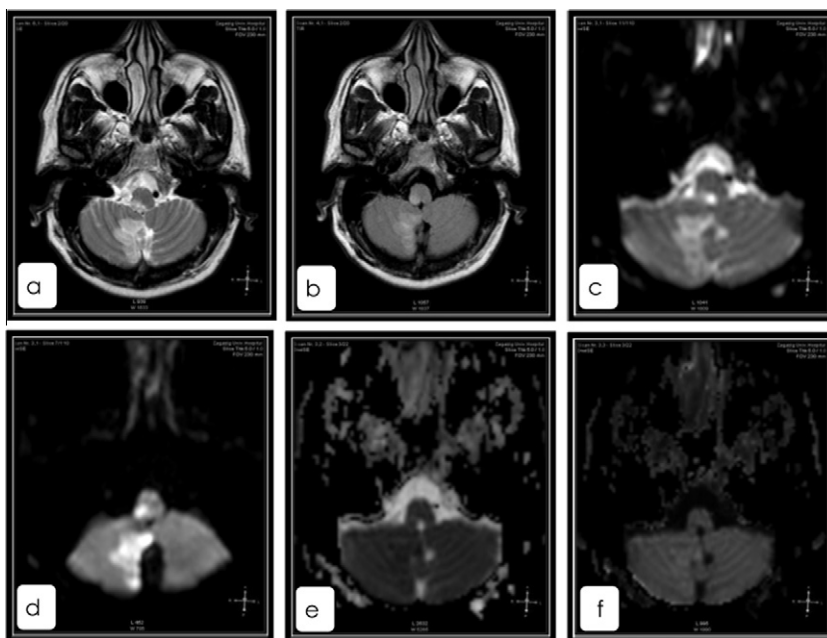
Our study (Table 1) agreed with the previous studies (14,28–32) regarding the evolution of ADC, DWI, and exponential signal intensity in different stages of infarction.

The exponential images have the advantage of showing the abnormal signal intensity because of restricted diffusion while negating the contribution of  $T_2$  signal intensity to diffusion-weighted images. These images retain the hyperintense signal characteristics of infarcts as seen on diffusion-weighted images to which radiologists have grown accustomed. Whereas on an ADC map, an acute infarct is seen as a hypointense region against an intermediate signal intensity background with relatively poor lesion conspicuity; on exponential images, an acute infarct is seen as a hyperintense lesion against a background of intermediate signal intensity normal brain tissue with high lesion conspicuity (17).

In one study (32) application of an IR pulse to suppress the CSF signal resulted in lower ADC values. This strongly suggests that the ADC values obtained from a conventional



**Fig. 7**  $T_2$  “shine through”. No abnormality could be detected at T2WI (a), FLAIR (b) images and ADC map (e). However, DWI-b = 0 (c) and DWI-b = 1000 (d) show hyperintense area in the left temporal region. At exponential image (f) the hyperintense left temporal area is no longer seen denoting  $T_2$  shine-through effect seen by DWI and eliminated by exponential image.



**Fig. 8** Late subacute infarction after 8 days of symptoms. Axial T2WI (a), FLAIR (b) and DWI-b = 0 (c) show two hyperintense areas of infarctions at the medial aspect of the right cerebellar hemisphere and right lateral aspect of the medulla oblongata. The lesions display high SI at DWI-b = 1000 (d) and intermediate SI at ADC map (e). At exponential image (f) it displays iso-intense signal denoting late subacute infarctions.

ADC map are contaminated with CSF signal, an issue first addressed by Pierpaoli et al. (33). Thus, the IR pulse may be required to obtain accurate ADC values. Moreover, chronic lesions are frequently better visualized on the

FLAIR ADC map than on the conventional ADC map (32).

On exponential images the removal of the  $T_2$  signal intensity contribution (Fig. 7) moderately lowered signal intensity

of infarcts compared with that on diffusion-weighted images, however, the lesion conspicuity was sufficient in all cases to allow identification of infarcts.

This agreed with our study, where the lesion conspicuity on exponential images alone (without DWI or ADC) was sufficient in all cases as we could detect and determine the different types of infarction in the examined patients.

Because only a single set of images is needed, exponential images are easier to use than a combination of trace diffusion-weighted images and ADC maps (17). In addition, because the contrast characteristics of exponential images are similar to those of diffusion-weighted images, the imaging findings are similar to those to which radiologists have grown accustomed. Finally, exponential images can be used to more precisely determine the presence of restricted water diffusion, which should help to increase the accuracy of estimating the age of cerebral infarcts (17). Exponential image offers a simple solution to the common pitfalls in DWI or ADC map (34).

In conclusion exponential image can detect area with restricted diffusion more accurately as it combines the advantages of both DWI and ADC, by removing the “T<sub>2</sub> shine-through effect” in DWI, and higher lesion conspicuity without CSF contamination seen on ADC. Image interpretation is much more easier if we use Exponential image, as one can revise a single set of images instead of two sets (DWI and ADC) with more familiar images (similar to DWI) and higher contrast (than on ADC). One can state at the moment that exponential image offers promising and reliable images that can replace both DWI and ADC in diagnosing patients with infarction.

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