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# Ligand-Specific Interactions Modulate Kinetic. **Energetic, and Mechanical Properties** of the Human $\beta_2$ Adrenergic Receptor

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#### **SUMMARY**

G protein-coupled receptors (GPCRs) are a class of versatile proteins that transduce signals across membranes. Extracellular stimuli induce inter- and intramolecular interactions that change the functional state of GPCRs and activate intracellular messenger molecules. How these interactions are established and how they modulate the functional state of GPCRs remain to be understood. We used dynamic single-molecule force spectroscopy to investigate how ligand binding modulates the energy landscape of the human  $\beta_2$  adrenergic receptor (β<sub>2</sub>AR). Five different ligands representing either agonists, inverse agonists or neutral antagonists established a complex network of interactions that tuned the kinetic, energetic, and mechanical properties of functionally important structural regions of β<sub>2</sub>AR. These interactions were specific to the efficacy profile of the ligands investigated and suggest that the functional modulation of GPCRs follows structurally well-defined interaction patterns.

### **INTRODUCTION**

G protein-coupled receptors (GPCRs) are a class of extraordinarily versatile molecules that transduce signals through cellular membranes. They respond to light, neurotransmitters, and hormones and are responsible for the senses of smell, taste, and sight. GPCRs are often described as bimodal switches that can exist in inactive and in active states. This simplified description provides only limited explanation of their complex functional behavior. For instance GPCRs can activate several G protein isoforms. Furthermore, they can trigger G protein-independent signaling pathways (Lefkowitz and Shenoy, 2005). Additionally, ligands that bind to GPCRs have distinct efficacy profiles, inducing different downstream signaling pathways. Structurally elucidating this dynamic functional behavior of GPCRs remains challenging. Recently, crystal structures of GPCRs in different functional states have been determined by Choe et al. (2011), Jaakola et al. (2008), Palczewsky et al. (2000), Rasmussen et al. (2007, 2011), Scheerer et al. (2008), Standfuss et al. (2011), and Warne et al. (2008). They suggest that binding of different ligands induces a variety of conformational and functional intermediates. In the unliganded state many GPCRs exhibit basal activity. Binding of agonists triggers a series of noncovalent intramolecular interactions, which lead to activation of the receptor. Interactions that stabilize the basal state of the receptor are disrupted, whereas interactions stabilizing active states are established (Ghanouni et al., 2001; Rosenbaum et al., 2009). Different combinations of these interactions, induced by structurally and chemically different ligands, modulate specific conformations that induce the functional intermediates involved in downstream signaling cascades.

GPCRs exhibiting a basal activity can activate their G protein even in the absence of agonists. Ligands that bind to GPCRs can either increase or decrease the basal activity, depending on their efficacy profile (Kenakin, 2002). A broad spectrum of ligands is available for GPCRs. Agonists are ligands that can activate the GPCR. Full agonists lead to maximal activation of the receptor, whereas partial agonists are not able to fully activate the GPCR, even at saturating concentrations. Inverse agonists decrease the basal activity, and neutral antagonists do not have any effect on the activity of the receptor. However, antagonists block the access of other ligands to the receptor. Depending on the ligand bound, the receptor can virtually exist in many states between fully active and fully inactive. This variety of ligand-specific conformational states explains the coexistence of multiple functional states of the receptor (Kobilka, 2011; Kobilka and Deupi, 2007).

The human  $\beta_2$  adrenergic GPCR ( $\beta_2$ AR) is one of the most extensively studied GPCRs. Besides the  $\alpha$  subfamily of adrenergic receptors (ARs), β<sub>2</sub>AR belongs to the class of A receptors (Caron and Lefkowitz, 1993). Several crystal structures of β<sub>2</sub>AR are available (Cherezov et al., 2007; Rasmussen et al., 2007, 2011; Rosenbaum et al., 2007, 2011). The  $\beta_2$  receptor mainly resides in smooth muscles (Barnes, 1993), binds the hormones adrenalin and noradrenalin, and is involved in regulating cardiovascular and pulmonary function. Several ligands that bind to β<sub>2</sub>AR are used as drugs in cardiac disease and asthma treatment (Bai, 1992). Investigating the interactions established by ligands and understanding the effect of ligand binding on the dynamic energy landscape of the receptor might help to improve the development of more efficient drugs.

Molecular interactions of membrane proteins like β<sub>2</sub>AR can be quantified and localized by atomic force microscopy (AFM)based single-molecule force spectroscopy (SMFS) (Kedrov



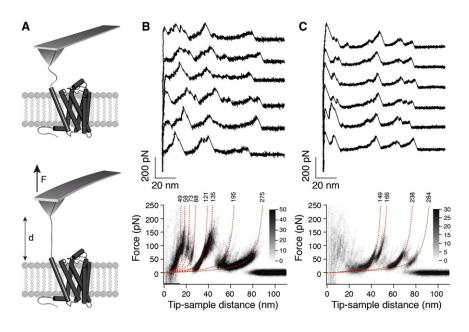


Figure 1. SMFS of β<sub>2</sub>AR Reconstituted into Liposomes Containing Phospholipids and Cholesterol

(A) Pushing the AFM stylus onto the proteoliposomes forces the unspecific attachment of the β<sub>2</sub>AR polypeptide to the stylus. Retraction of the cantilever stretches the polypeptide attached to the AFM stylus and induces the sequential unfolding of the receptor. F, force; d, distance. (B and C) Selection of F-D curves recorded upon N-terminal (B, top) and C-terminal (C, top) unfolding of β<sub>2</sub>AR. Superimpositions of 103 (B, bottom) and 56 (C, bottom) F-D curves highlight their common features. Red lines represent WLC curves fitting the main force peaks with the number on top indicating the average contour lengths (in amino acids) revealed from the fits. Gray scale bars allow evaluating how frequently individual force peaks were populated. See also Figures S1 and S2.

et al., 2007a). Once these interactions have been assigned to secondary structure elements, parameters describing the energy landscape of the membrane protein can be determined by dynamic SMFS (DFS) (Janovjak et al., 2008). Previously, SMFS and DFS have been applied to elucidate ligand and inhibitor binding to bacterial transmembrane transporters (Bippes et al., 2009; Ge et al., 2011; Kedrov et al., 2005, 2008) and yeast mitochondrial carriers (Kedrov et al., 2010). Here, we use SMFS and DFS to determine interactions and energy barriers that are established in human  $\beta_2AR$  and change after binding of ligands with different efficacy profiles. To ensure native-like conditions, the receptor has been reconstituted into phospholipid liposomes containing the cholesterol analog cholesteryl hemisuccinate (CHS). Several ligands (three agonists, one inverse agonist, one neutral antagonist) were tested. Changes in energetic, kinetic, and mechanical properties of structural segments of the receptor unravel the complexity of the interaction network that determines the conformational and functional state of  $\beta_2AR$ .

#### **RESULTS**

# Mechanical Unfolding of Human $\beta_2AR$

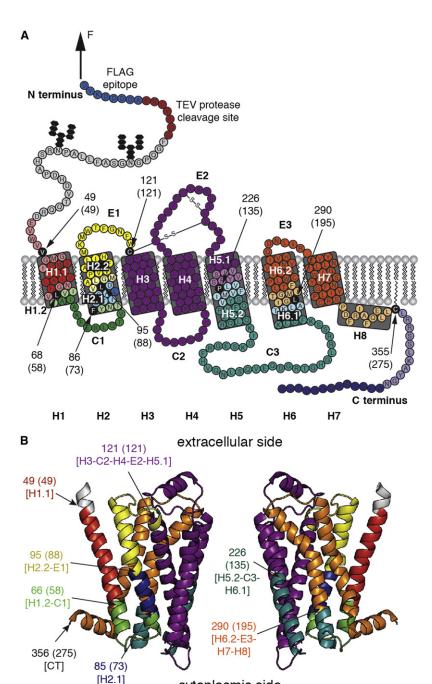
To determine interactions in native-like  $\beta_2AR$ , proteoliposomes containing  $\beta_2AR$  were adsorbed onto freshly cleaved mica and imaged by AFM in buffer solution (Müller and Engel, 2007). The AFM topographs showed  $\beta_2AR$  proteoliposomes densely covering the supporting mica (see Figure S1 available online). To nonspecifically attach single  $\beta_2AR$  to the AFM stylus, the stylus was pushed onto the proteoliposomes reaching a force of  $\sim$ 700 pN for 0.5 s (Müller and Engel, 2007). Upon withdrawal of the stylus, the receptor was mechanically stressed, and forcedistance (F-D) curves were recorded (Figure 1A). Principally,  $\beta_2AR$  could adhere to the AFM stylus with every polypeptide loop or terminal end. Only when pulling either the N-terminal or C-terminal end and upon unfolding  $\beta_2AR$  into a fully stretched conformation did the F-D curves reach maximal lengths. For analysis, only F-D curves were selected, whose lengths corre-

sponded to that of fully unfolded and stretched  $\beta_2AR$  polypeptides ( $\sim$ 70–90 nm; see Experimental Procedures). About 0.5% of  $\sim$ 1,120,000 F-D curves showed reproducible force peak patterns that extended over the length of a fully unfolded  $\beta_2AR$  molecule (Figures 1B and 1C). Although the F-D curves looked similar, individual curves could differ to some extent from each other. Two major classes of F-D curves were observed (Figures 1B and 1C). To highlight common force peaks among the F-D curves, they were superimposed and converted into density plots. Each force peak of a F-D curve represents the unfolding of a structural segment of the receptor (Kedrov et al., 2007a). The magnitude of the force peak corresponds to the strength of the interaction that stabilizes a structural segment against unfolding. Such an interaction is composed of inter- and intramolecular interactions.

### Unfolding β<sub>2</sub>AR from N- and C-Terminal Ends

We assumed that the two classes of F-D curves (Figures 1B and 1C) corresponded to mechanically unfolding the receptor from the N- and C-terminal end. To assign these classes to N- or C-terminal unfolding, the N-terminal FLAG tag was enzymatically removed, and the shortened  $\beta_2AR$  was unfolded (Figure S2). A shift of  $\sim$ 14 aa was observed in one class of F-D curves, suggesting that this particular class corresponds to N-terminal unfolding. Approximately 75% of  $\sim$ 5,600 F-D curves corresponded to the unfolding of β<sub>2</sub>AR by mechanically pulling the N-terminal end (Figure 1B). The remaining 25% of the F-D curves represented unfolding the receptor from the C-terminal end (Figure 1C). Superimpositions of F-D curves showed a characteristic pattern of eight force peaks when unfolding  $\beta_2AR$  from the N-terminal end (Figure 1B). When unfolding  $\beta_2AR$  from the C-terminal end, only four force peaks were detected. The C-terminal region of the receptor, which is unfolded at pulling distances <30 nm, did not reveal reproducible unfolding events (force peaks) (Figure 1C). Due to the low occurrence of C-terminally pulled F-D curves that, in addition, showed less reproducible force peaks, we focused our analysis on F-D curves pulled from the N-terminal end.





# **Interactions Stabilize Distinct Structural Segments**

When exerting a mechanical pulling force to a terminal end, β<sub>2</sub>AR unfolds in sequential steps that are reflected by individual force peaks of a F-D curve (Figure 1). Every force peak was fitted using the worm-like chain (WLC) model (Experimental Procedures) to reveal the contour length of the unfolded polypeptide that connected AFM stylus and the unfolding intermediate of the receptor. The contour lengths of all force peaks allowed determining all unfolding steps of  $\beta_2$ AR (Figure 1; Table S1). An unfolding step, in which a structural segment unfolds, describes the

cytoplasmic side

#### Figure 2. Structural Segments Stabilizing the Human β<sub>2</sub>AR

Secondary (A) and tertiary (B) structure model of β<sub>2</sub>AR is shown. Each color represents a structural segment that is stabilized by inter- and intramolecular interactions. (A) Black amino acids highlight the end of the previous and the beginning of the next stable structural segment. This structural position corresponds to the mean contour length (given in brackets) revealed from the WLC fitting of reproducibly detected force peaks in Figure 1B. Amino acids colored at less intensity give the SD of the average force peak (Table S1). In case the end/beginning of a structural segment had to be assumed to lie within the membrane or at the membrane surface opposite to the pulling AFM stylus, a certain number of amino acids were added to the contour length to structurally locate the segment (Experimental Procedures). All seven transmembrane  $\alpha$  helices of  $\beta_2AR$  are labeled H1-H7. Cytoplasmic and extracellular loops are indicated as C1, C2, C3, and E1, E2, E3, respectively. H8 denotes the short C-terminal helix 8 at the cytoplasmic side. The secondary structural model (A) of C-terminal truncated β<sub>2</sub>AR carrying a N-terminal FLAG epitope (blue) followed by a TEV protease cleavage site (green) was taken from Rasmussen et al. (2007). The tertiary structural model (B) was taken from PDB ID 2RH1. See also Figure S3 and Table S1.

transfer of one unfolding intermediate to the next (Kedrov et al., 2007a). In the first unfolding step, the N-terminal transmembrane  $\alpha$  helix of β<sub>2</sub>AR unfolds. After this, the polypeptide linking the AFM stylus and β<sub>2</sub>AR is elongated and stretched again when encountering the next interaction stabilizing a structural segment of the unfolding receptor. This stepwise unfolding continues until the entire receptor unfolded. We detected eight unfolding steps, each one describing the unfolding of a structural segment stabilized by the  $\beta_2AR$  molecule. Mapped onto the secondary structure, these stable structural segments show where inter- and intramolecular interactions stabilized the receptor (Figure 2).

## **Determining Energetic, Kinetic, and** Mechanical Properties Stabilizing β<sub>2</sub>AR in the Absence and Presence of Ligands

The force required to unfold a structural segment reflects the strength of interactions stabilizing the segment. This interaction strength

depends on the loading rate (pulling force applied versus time) at which the structural segment is forced to unfold (Evans, 2001). Therefore, the unfolding force gives only a relative measure of the stability of a structure exposed to mechanical stress. However, the free energy unfolding barrier describes the kinetic and mechanical stability of a folded structure at equilibrium (Figure 3A). Parameters characterizing this energy barrier can be approximated using DFS. To reveal these parameters, DFS determines the most probable interaction strengths that stabilize every structural segment over a wide range of loading rates (Evans, 2001; Janovjak et al., 2008).



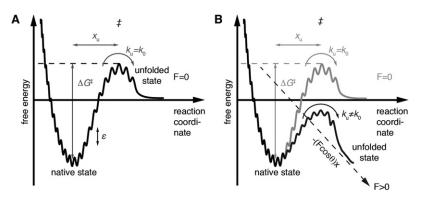


Figure 3. Free Energy Unfolding Landscape Describing Energetic and Kinetic Parameters of Stable Structural Segments

(A) According to the Bell-Evans model of Evans (1998, 2001), folded structures can be characterized using a simple two-state model. The native, folded structure resides in an energy valley and is separated by an energy barrier from the unfolded state. As approximated previously the surface roughness of the energy landscape of transmembrane  $\alpha$  helices,  $\epsilon$ , is  $\sim\!\!4\text{--}6~k_BT$  (Janovjak et al., 2007). This roughness creates local energy minima that can stabilize functionally related conformational states of a structural segment. Thus, for a given surface roughness, a wide energy valley can host more conformational states (i.e., hosts a higher conformational variability) of a structural segment compared to a narrow energy valley.

The transition state (‡) must be overcome to induce unfolding.  $x_u$  represents the distance between the folded state and the transition state,  $k_0$  is the transition rate for crossing the energy barrier under zero force, and  $\Delta G^{\ddagger}$  gives the activation energy for unfolding the segment.

(B) Applying an external force (F) changes the thermal likelihood of reaching the top of the energy barrier. The energy profile along the reaction coordinate (pulling direction) is tilted by the mechanical energy -(Fcos $\theta$ )x, as indicated by the dashed line. The applied force does not change the ground-to-transition state distance  $x_u$ .  $\theta$  describes the angle of the externally applied force relative to the reaction coordinate. As a result of this tilt, the energy barrier separating the folded from the unfolded state decreases, and the probability of the folded structural segment to unfold increases.

We determined the most probable unfolding force of every structural segment at different loading rates. F-D curves were recorded at seven pulling velocities (100, 300, 600, 900, 1,200, 2,500, and 5,000 nm/s) (Figure S4). To investigate to what extent the binding of different ligands affects the energy landscape of  $\beta_2$ AR, DFS was carried out in the unbound state and in the presence of the synthetic agonists BI-167107 (BI, Boehringer Ingelheim) and THRX-144877 (THRX, Theravance), the natural agonist adrenalin, the inverse agonist carazolol, and the neutral antagonist alprenolol. For all pulling velocities superimpositions of the F-D curves did not change drastically upon ligand binding to  $\beta_2$ AR (Figures S4 and S5). Next, we determined the most probable unfolding force ( $F^*$ ) of every force peak characterizing a stable structural segment of  $\beta_2$ AR and plotted them for the different loading rates ( $r_f^*$ ) (Figure 4).

### Ligands Change Energy Landscape of β<sub>2</sub>AR

As predicted by Evans (1998) and Evans and Ritchie (1997) and experimentally verified using membrane proteins by Bippes et al. (2009), Janovjak et al. (2004), Kawamura et al. (2010), Kedrov et al. (2008), Sapra et al. (2008a, 2008b), increasing the loading rate led to increased unfolding forces. The linear relationship between the most probable rupture force and the logarithm of the loading rate suggests a single energy barrier separating the folded from unfolded state for every structural segment (Evans and Ritchie, 1997). Fitting the DFS plots (Figure 4) using Equation 1 revealed the distance between ground and transition state  $(x_u)$ , transition rate  $(k_0)$ , free energy  $(\Delta G^{\ddagger})$ , and mechanical spring constant (κ) of every structural segment (Figure 2). Differences between these parameters imply that the kinetic stability and mechanical nature of molecular interactions changed in the presence of ligands. To determine the statistical significance of these differences, DFS plots from ligand-free and ligandbound β<sub>2</sub>AR were fitted simultaneously, resulting in a common estimate for  $x_u$  and  $k_0$ . The sum of squares of both separate and simultaneous fits was assessed by an F test (Table S2) (Motulsky and Christopoulos, 2004). Several segments showed statistically significant differences after ligand binding (Table 1). In the following we will describe the significant differences detected in our experiments.

## Structural Segments Changing Conformational Variability upon Ligand Binding

The distance between ground state and transition state  $x_{ij}$ approximates the conformational variability of a structure (Figure 3) (Kumar et al., 2000). If a narrow energy valley stabilizing a structural segment becomes wider after binding of a ligand, the ligand increases the number of conformational states (i.e., conformational variability) the structural segment can adopt. Such an effect was observed upon ligand binding to β<sub>2</sub>AR (Table 1). Binding of agonists (BI, THRX, or adrenalin) significantly increased the conformational variability of the core segment [H3-C2-H4-E2-H5.1] (p < 0.001), carazolol significantly increased the conformational variability of structural segments [H1.2-C1] (p < 0.001), [H3-C2-H4-E2-H5.1] (p < 0.001), and [H6.2-E3-H7-H8] (p < 0.05), whereas alprenolol significantly increased the conformational variability of [H1.1] (p < 0.05) (Table 1). These results show that ligand binding increases the conformational variability (or states) of certain structural regions of β<sub>2</sub>AR, whereas all other structural regions were not affected significantly. It appeared that some structural regions were modulated by different ligands, whereas other regions were modulated by only one ligand. However, to what extent the conformational variability of a structural region changed was specific to the ligand.

# Structural Segments Changing Lifetime upon Ligand Binding

The transition rate  $k_0$  measures the lifetime (reciprocal of transition rate) of a structural segment. The DFS experiments (Table 1) detected that BI, THRX, or adrenalin binding significantly increased the lifetime of the structural segment [H3-C2-H4-E2-H5.1] (p < 0.001), that carazolol binding significantly increased the lifetime of the structural segments [H1.2-C1] (p < 0.001), [H2.1] (p < 0.05), [H3-C2-H4-E2-H5.1] (p < 0.001), and [H6.2-E3-H7-H8] (p < 0.05) and that alprenolol binding significantly



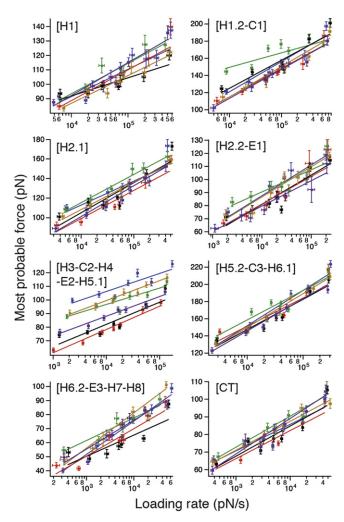


Figure 4. DFS Plots Reveal Loading Rate-Dependent Interactions Stabilizing BoAR

For each stable structural segment of β<sub>2</sub>AR, the most probable unfolding force was plotted against the loading rate. DFS fits using Equation 1 are shown for unliganded (red), alprenolol-bound (black), carazolol-bound (green), BIbound (blue), THRX-bound (orange), and adrenalin-bound (violet) states. Values for  $x_u$  and  $k_0$  obtained from fitting the DFS plots are given in Table 1. Error bars represent the SE of most probable force and loading rate. See also Figures S4 and S5.

increased the lifetime of the structural segment [H1.1] (p < 0.05) (Table 1). These results demonstrate that ligand binding changes the kinetic properties of structural regions within  $\beta_2$ AR. However, to what extent the kinetic properties of a structural region changed was again specific to the ligand.

## **Structural Segments Changing Free Energy upon Ligand Binding**

The free energy  $\Delta G^{\ddagger}$  characterizes the height of the energy barrier stabilizing a folded structure (Figure 3). DFS measurements showed that ligand binding increased the free energy of several structural segments (Table 1). BI, THRX, and adrenalin binding significantly increased  $\Delta G^{\ddagger}$  of structural segment [H3-C2-H4-E2-H5.1] (p < 0.001), carazolol significantly increased  $\Delta G^{\ddagger}$  of structural segments [H1.2-C1] (p < 0.001), [H2.1] (p < 0.05), [H3-C2-H4-E2-H5.1] (p < 0.001), and [H6.2-E3-H7-H8] (p < 0.05), and alprenolol significantly increased  $\Delta G^{\ddagger}$  of structural segment [H1.1] (p < 0.05).

# **Structural Segments Changing Mechanical Properties** upon Ligand Binding

Similar to the other parameters characterizing the energy barriers, the k values that quantify the mechanical rigidity of structural segments (Dietz et al., 2006) changed upon ligand binding (Table 1). Binding of the agonists BI, THRX, and adrenalin significantly increased the mechanical elasticity of the core structural segment [H3-C2-H4-E2-H5.1] (p < 0.001), and alprenolol significantly decreased the mechanical elasticity of structural segment [H1.1] (p < 0.05). Carazolol significantly increased the mechanical elasticity of structural segments [H1.2-C1] (p < 0.001), [H3-C2-H4-E2-H5.1] (p < 0.001), and [H6.2-E3-H7-  $\,$ H8] (p < 0.05) and decreased that of structural segment [H2.1] (p < 0.05). These results showed that the binding of a ligand changed the mechanical properties of certain structural regions.

#### **DISCUSSION**

# Ligand Binding to β<sub>2</sub>AR Lacks Pronounced Localized

As for all membrane proteins investigated so far by SMFS (Bippes and Muller, 2011), the F-D spectra recorded during mechanical unfolding of native-like β<sub>2</sub>AR reconstituted into proteoliposomes showed a reproducible pattern of force peaks (Figures 1B and 1C). The reproducibility of the force peak pattern suggests that β<sub>2</sub>AR establishes a characteristic interaction network (Kedrov et al., 2007a). Ligand binding to the receptor did not establish additional force peaks or significantly modify the strength of existing force peaks (Figures S4 and S5). In contrast, SMFS detected a significantly increased force peak after ligand binding to functionally activated Na<sup>+</sup>/H<sup>+</sup> antiporters NhaA from Escherichia coli and MjHhaP1 from Methanococcus jannaschii (Kedrov et al., 2005, 2007b). The increasing interaction force was correlated to specific interactions established between the ligand Na+ and the deprotonated aspartic acid residues at the Na<sup>+</sup>-binding site. In β<sub>2</sub>AR multiple amino acid residues from several transmembrane  $\alpha$  helices contribute to ligand binding (Rasmussen et al., 2011; Rosenbaum et al., 2007). Thus, it is expected that ligand binding modulates the functional state of β<sub>2</sub>AR by changing the interaction network in the GPCR (Kobilka and Deupi, 2007). However, because we did not observe drastic changes of the force peak pattern such as observed for other membrane proteins after ligand binding (Kedrov et al., 2005, 2007b), we conclude that ligand binding established rather small changes to the interactions that structurally stabilize  $\beta_2AR$  in the unliganded conformation.

## **Conformational Variability and Kinetic Stability** of Unliganded β<sub>2</sub>AR

DFS studies suggest that structural segments of bacteriorhodopsin, bovine and mouse rhodopsin, the antiporter NhaA, and the transporter BetP are stabilized by single energy barriers (Figure 3) (Ge et al., 2011; Janovjak et al., 2004; Kawamura et al., 2010; Kedrov et al., 2008; Sapra et al., 2008c). We made



Table 1. Parameters Characterizing Energy Barriers and Mechanical Spring Constants of Structural Segments Stabilizing β <sub>2</sub> AR						
Stable Structural Segment	Unliganded β <sub>2</sub> AR	Agonist (BI)	Agonist (THRX)	Agonist (Adrenalin)	Inverse Agonist (Carazolol)	Neutral Antagonist (Alprenolol)
	$x_u \pm SD (nm)$					
[H1.1]	$0.44 \pm 0.04$	$0.50 \pm 0.05$	$0.49 \pm 0.07$	$0.47 \pm 0.05$	$0.45 \pm 0.04$	$0.75 \pm 0.12^{a}$
[H1.2-C1]	$0.29 \pm 0.02$	$0.27 \pm 0.02$	$0.30 \pm 0.04$	$0.26 \pm 0.03$	$0.56 \pm 0.07^{a}$	0.29 ± 0.02
[H2.1]	$0.33 \pm 0.02$	$0.39 \pm 0.04$	$0.39 \pm 0.05$	$0.33 \pm 0.04$	$0.33 \pm 0.02$	0.31 ± 0.02
[H2.2-E1]	$0.45 \pm 0.05$	$0.40 \pm 0.04$	$0.40 \pm 0.06$	$0.54 \pm 0.08$	$0.56 \pm 0.08$	$0.42 \pm 0.03$
[H3-C2-H4-E2-H5.1]	$0.55 \pm 0.03$	$0.71 \pm 0.07^{a}$	$0.73 \pm 0.13^{a}$	$0.65 \pm 0.09^{a}$	$0.79 \pm 0.08^{a}$	$0.58 \pm 0.04$
[H5.2-C3-H6.1]	$0.29 \pm 0.02$	$0.23 \pm 0.01$	0.25 ± 0.02	$0.26 \pm 0.02$	$0.28 \pm 0.02$	0.27 ± 0.02
[H6.2-E3-H7-H8]	$0.49 \pm 0.03$	$0.40 \pm 0.02$	$0.39 \pm 0.05$	$0.40 \pm 0.04$	$0.59 \pm 0.06^{a}$	$0.58 \pm 0.05$
[CT]	$0.59 \pm 0.05$	$0.63 \pm 0.06$	$0.64 \pm 0.10$	$0.49 \pm 0.06$	$0.54 \pm 0.05$	$0.55 \pm 0.04$
	$k_0 \pm SD (10^{-3} s^{-1})$					
[H1.1]	77.3 ± 72.5	18.7 ± 22.0	43.8 ± 64.7	26.6 ± 30.5	41.5 ± 33.9	0.09 ± 0.26 <sup>a</sup>
[H1.2-C1]	248 ± 178	253 ± 161	121 ± 147	473 ± 372	$0.002 \pm 0.005^{a}$	111 ± 76.2
[H2.1]	290 ± 174	23.1 ± 27.1	30.5 ± 42.1	234 ± 210	$80.8 \pm 54.8^{a}$	290 ± 179
[H2.2-E1]	166 ± 140	196 ± 144	211 ± 236	38.2 ± 55.2	6.61 ± 11.5	261 ± 155
[H3-C2-H4-E2-H5.1]	38.8 ± 22.4	$0.02 \pm 0.03^{a}$	$0.04 \pm 0.01^{a}$	1.51 ± 2.75 <sup>a</sup>	$0.02 \pm 0.03^{a}$	13.4 ± 10.4
[H5.2-C3-H6.1]	18.0 ± 13.5	118 ± 53.3	58.3 ± 41.1	59.5 ± 41.4	16.7 ± 11.5	44.5 ± 24.8
[H6.2-E3-H7-H8]	320 ± 118	663 ± 184	480 ± 300	636 ± 329	$21.9 \pm 20.7^{a}$	151 ± 106
[СТ]	10.7 ± 7.98	$3.28 \pm 3.21$	2.55 ± 4.06	33.0 ± 31.2	$9.99 \pm 8.90$	15.4 ± 10.8
	$\Delta G^{\ddagger} \pm SD (k_B T)$					
[H1.1]	21.0 ± 0.9	22.4 ± 1.2	21.5 ± 1.5	22.0 ± 1.1	21.6 ± 0.8	27.7 ± 2.7 <sup>a</sup>
[H1.2-C1]	19.8 ± 0.7	$19.8 \pm 0.6$	20.5 ± 1.2	19.2 ± 0.8	$31.5 \pm 2.5^{a}$	20.6 ± 0.7
[H2.1]	19.7 ± 0.6	22.2 ± 1.2	21.9 ± 1.4	19.9 ± 0.9	$20.9 \pm 0.7^{a}$	19.7 ± 0.6
[H2.2-E1]	20.2 ± 0.8	$20.1 \pm 0.7$	20.0 ± 1.1	21.7 ± 1.4	23.4 ± 1.7	19.8 ± 0.6
[H3-C2-H4-E2-H5.1]	21.7 ± 0.6	$29.4 \pm 1.7^{a}$	$28.6 \pm 2.9^{a}$	24.9 ± 1.8 <sup>a</sup>	$29.3 \pm 1.7^{a}$	22.7 ± 0.8
[H5.2-C3-H6.1]	$22.4 \pm 0.8$	$20.6 \pm 0.5$	21.3 ± 0.7	21.2 ± 0.7	$22.5 \pm 0.7$	21.5 ± 0.6
[H6.2-E3-H7-H8]	$19.6 \pm 0.4$	$18.8 \pm 0.3$	19.2 ± 0.6	18.9 ± 0.5	$22.2 \pm 0.9^{a}$	20.3 ± 0.7
[CT]	23.0 ± 0.7	24.1 ± 1.0	24.4 ± 1.6	21.8 ± 0.9	$23.0 \pm 0.9$	22.6 ± 0.7
	κ ± SD (N/m)	'	<u> </u>			
[H1.1]	0.88 ± 0.13	0.74 ± 0.12	0.76 ± 0.17	0.83 ± 0.14	0.88 ± 0.12	$0.40 \pm 0.09^{a}$
[H1.2-C1]	2.02 ± 0.26	2.28 ± 0.26	1.84 ± 0.39	2.30 ± 0.40	$0.83 \pm 0.13^{a}$	2.04 ± 0.22
[H2.1]	1.49 ± 0.18	1.22 ± 0.20	1.19 ± 0.25	1.50 ± 0.27	$1.60 \pm 0.16^{a}$	1.71 ± 0.20
[H2.2-E1]	0.84 ± 0.15	1.03 ± 0.15	1.04 ± 0.25	0.61 ± 0.15	0.62 ± 0.14	0.92 ± 0.10
[H3-C2-H4-E2-H5.1]	0.59 ± 0.06	$0.48 \pm 0.06^{a}$	0.44 ± 0.11 <sup>a</sup>	0.49 ± 0.11 <sup>a</sup>	$0.39 \pm 0.05^{a}$	0.56 ± 0.06
[H5.2-C3-H6.1]	2.23 ± 0.25	3.21 ± 0.26	2.71 ± 0.34	2.53 ± 0.33	$2.45 \pm 0.24$	2.47 ± 0.22
[H6.2-E3-H7-H8]	0.69 ± 0.08	$0.98 \pm 0.09$	1.03 ± 0.20	0.99 ± 0.19	$0.53 \pm 0.09^{a}$	0.50 ± 0.08
[CT]	$0.54 \pm 0.06$	$0.51 \pm 0.07$	0.49 ± 0.11	0.75 ± 0.14	$0.66 \pm 0.09$	0.61 ± 0.07

Parameters are shown for unliganded  $\beta_2AR$  and in the presence of two high-affinity agonists (BI and THRX), a strong partial agonist (adrenalin), an inverse agonist (carazolol), and a neutral antagonist (alprenolol). Errors represent SDs. See also Table S1. <sup>a</sup>Statistically significant changes to the unliganded state as assessed by F tests (Table S2).

the same observation for the structural segments of  $\beta_2AR$ . The transition state distance  $x_u$  separating the folded from the unfolded state of every structural segment of  $\beta_2AR$  ranged from 0.3 to 0.6 nm (Table 1). Thus, the structural segments of  $\beta_2AR$  must be stretched by  $\sim$ 0.3–0.6 nm to induce unfolding. These rather short distances suggest that short-ranged interand intramolecular bonds, such as hydrogen bonds, van der Waals interactions, or electrostatic interactions, had to be ruptured to induce unfolding of the receptor. On average the transition state distance of structural segments determined of

 $\beta_2$ AR was similar to the average values of  $\sim$ 0.4 nm determined for structural segments stabilizing bacteriorhodopsin, bovine rhodopsin, and NhaA ( $x_u$  ranging from 0.2 to 0.8 nm) (Janovjak et al., 2004; Kawamura et al., 2010; Kedrov et al., 2008; Sapra et al., 2008c). The structural segments of unliganded  $\beta_2$ AR revealed transition rates  $k_0$  between 0.011 and 0.320 s<sup>-1</sup> (Table 1), indicating lifetimes ranging between  $\sim$ 3 and  $\sim$ 90 s. These transition rates were in the range of those measured for other membrane proteins ranging from 0.001 to 0.9 s<sup>-1</sup> (Janovjak et al., 2004; Kawamura et al., 2010; Kedrov et al., 2008; Sapra



et al., 2008c). However, the  $k_0$  values of the structural segments of  $\beta_2 AR$  differed by a factor of 30 with structural segments [H1.1], [H3-C2-H4-E2-H5.1], and [CT] representing the kinetically stable regions and [H1.2-C1], [H2.1], and [H6.2-E3-H7-H8] the kinetically less stable ones. Biophysical and functional studies support a multistate model of β<sub>2</sub>AR in the absence of ligands (Deupi and Kobilka, 2010). These multiple conformational and functional states observed for unliganded β<sub>2</sub>AR may be directly related to the conformational variability and kinetic heterogeneity of the receptor's structural segments observed by DFS.

# **Energetic Stability and Mechanical Elasticity** of Unliganded β<sub>2</sub>AR

The free energy barrier  $\Delta G^{\ddagger}$  stabilizing the structural segments of unliganded  $\beta_2$ AR ranged from  $\sim$ 20 to 23  $k_BT$ . These free energy differences were below that determined for structural segments of bovine rhodopsin in the inactive dark state ( $\Delta G^{\ddagger}$  between 20 and 28  $k_BT$ ) (Table S3) and below those determined for the structurally similar but functionally different bacteriorhodopsin  $(\Delta G^{\ddagger})$  between 21 and 29  $k_BT$ ) (Kawamura et al., 2010; Sapra et al., 2008c). Thus, the structural segments of unliganded  $\beta_2 AR$  were energetically less stable compared to those of bovine rhodopsin and bacteriorhodopsin.

Spring constants characterizing the mechanical elasticity of structural segments in the unliganded state varied by a factor of four (Table 1). The intracellular end of  $\alpha$  helix H1 together with the first intracellular loop [H1.2-C1] ( $\kappa$  = 2.02 N/m) and the structural segment [H5.2-H6.1-C3] ( $\kappa$  = 2.23 N/m) formed the most rigid structures of the receptor. In contrast the core segment [H3-C2-H4-E2-H5.1] ( $\kappa$  = 0.59 N/m) and the C-terminal domain [CT] ( $\kappa$  = 0.54 N/m) formed the most elastic segments. In general the structural segments stabilizing  $\beta_2AR$  were more elastic compared to the structural segments of bacteriorhodopsin, where the values for κ ranged from 0.9 to 4.2 N/m (Sapra et al., 2008c). Compared to the elasticity of the structural segments of bovine rhodopsin (κ between 0.16 and 2.54 N/m) (Kawamura et al., 2010), the values observed for  $\beta_2AR$  were more similar, indicating that both class A GPCRs share consistent mechanical properties (Table S3). However, the spring constants of the structural core segments [H3-C2-H4-E2-H5.1] of both GPCRs differed from each other. In the case of unliganded  $\beta_2AR$ ,  $\kappa$  was about four times lower than  $\kappa$  of bovine rhodopsin in the dark state.

# **High Conformational Variability and Mechanical** Elasticity of Structural Core Correlate to Basal β<sub>2</sub>AR **Activity**

Parameters characterizing the energy barrier stabilizing unliganded β<sub>2</sub>AR describe the receptor in its basal and low-energy state (Kobilka and Deupi, 2007). It has been suggested that the basal activity of  $\beta_2AR$  in the absence of ligands may be attributed to an inherent structural flexibility and tendency to adopt several conformational states (Kobilka and Deupi, 2007). In our measurements the largest segment in the receptor core [H3-C2-H4-E2-H5.1] exposed a relatively high conformational variability (high  $x_{ij}$ ) and high mechanical elasticity (low  $\kappa$ ) compared to the other structural segments of  $\beta_2AR$  and compared to the core segment of the GPCR bovine rhodopsin in the dark state. This dark state of rhodopsin is stabilized by the covalently bound chromophore that acts as inverse agonist and traps the GPCRs in the inactive state (Zhukovsky and Oprian, 1989). Because the core segment of β<sub>2</sub>AR contains multiple ligand-binding sites (Rasmussen et al., 2011; Rosenbaum et al., 2007), the increased conformational variability and mechanical elasticity allow the core to sample more conformational states required to interact with a variety of different ligands. Thus, our DFS experiments suggest that the high conformational variability and mechanical elasticity of the core segment (Table 1) contribute to the basal activity of β<sub>2</sub>AR and favor ligand binding.

# Properties of $\beta_2$ AR Modified by the Neutral Antagonist **Alprenolol**

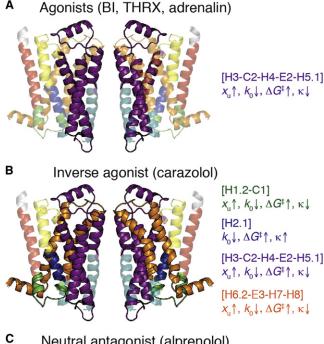
Neutral antagonists bind in the orthosteric pocket of a GPCR but have little or no effect on basal activity. In contrast to all other ligands tested, the neutral antagonist alprenolol only modulated the N-terminal region of transmembrane  $\alpha$  helix H1 ([H1.1]) and widened the energy valley  $x_u$  from 0.44 nm (unliganded) to 0.75 nm. Thus, alprenolol enhanced the conformational variability of the extracellular half of  $\alpha$  helix H1. Furthermore, binding of alprenolol significantly reduced the transition rate  $k_0$  and increased the lifetime of structural segment [H1.1]. The free energy  $\Delta G^{\ddagger}$ -stabilizing structural segment [H1.1] increased by  $\sim$ 7  $k_BT$ , whereas the spring constant  $\kappa$  decreased to 0.40 N/m (0.88 N/m in the unliganded state). These changes show that alprenolol kinetically and energetically stabilizes the extracellular part of α helix H1 and enhances its mechanical elasticity. Available crystal structures do not explain these observations. It has been suggested that  $\alpha$  helix H1 is involved in receptor silencing by oligomerization (Guo et al., 2008; Liang et al., 2003). Therefore, it may be speculated that the alprenololinduced kinetic and energetic stabilization as well as the structural softening of the extracellular half of  $\alpha$  helix H1 favor oligomerization of the receptor.

Although the affinity of alprenolol ( $K_D \sim 1$  nM) is comparable to that of the agonist THRX and greater than that of adrenalin, binding of the neutral antagonist did not show any effects on the structural core segment [H3-C2-H4-E2-H5.1]. Thus, alprenolol establishes very different interactions compared to THRX and to other agonists (Table 1). A possible explanation for this quite unique interaction pattern established in β<sub>2</sub>AR could be that alprenolol has a single aromatic ring that cannot establish strong interactions with F193 of loop E2, as shown by molecular dynamics docking simulations by Bokoch et al. (2010). Moreover, in contrast to both agonists and carazolol, alprenolol does not form polar interactions with serine residues from  $\alpha$  helix H5. This may explain that alprenolol cannot establish interactions at the core segment that are supposed to change the activity of  $\beta_2AR$ . In summary the DFS measurements unravel how a neutral antagonist works by simply constricting the access of other ligands to the receptor (Kenakin, 2008) and avoiding interactions at functionally important regions.

# An Overall Scheme: Most Ligands Modulate the Structural Core Segment of β<sub>2</sub>AR

To investigate to what extent ligands change the energetic, kinetic, and mechanical properties of  $\beta_2AR$ , we applied DFS in the presence of the synthetic agonists BI and THRX, the natural agonist adrenalin, the inverse agonist carazolol, or the neutral







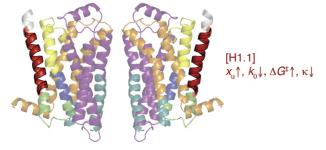


Figure 5. Structural Segments of β<sub>2</sub>AR Changing Properties upon

Structural segments that significantly change their energetic, kinetic, and mechanical properties upon binding of BI, THRX, or adrenalin (A), carazolol (B), and alprenolol (C) are highlighted (β<sub>2</sub>AR structure PDB ID code 2RH1). Arrows denote increasing (arrow up) and decreasing (arrow down) parameters characterizing the width of the energy valley  $(x_u)$ , transition rate  $(k_0)$ , energy barrier  $(\Delta G^{\ddagger})$ , and spring constant (k) of stable structural segments. Trends were taken from Table 1.

antagonist alprenolol. Figure 5 highlights which ligands modulate the properties of different structural segments of  $\beta_2AR$ . Binding of both agonists and the inverse agonist carazolol significantly modified the energetic, kinetic, and mechanical parameters of the structural core segment [H3-C2-H4-E2-H5.1]. The magnitude of the effect correlates relatively well with ligand affinity, with the lowest values being observed for the highest affinity ligands. This may be explained by extensive interactions between ligands and transmembrane  $\alpha$  helices H3 and H5. As noted above, the small effect observed for the neutral antagonist alprenolol may be explained by the absence of polar interactions between alprenolol and transmembrane  $\alpha$  helix H5. In the presence of agonists and carazolol, the energy valley stabilizing the structural core segment increased its distance to the transition state  $x_u$  from 0.55 nm (unliganded  $\beta_2AR$ ) to 0.73 nm (THRX), 0.71 nm (BI), 0.65 nm (adrenalin), and 0.79 nm (carazolol). This shift toward wider energy valleys in these ligand-bound states implies that the core segment [H3-C2-H4-E2-H5.1] increases conformational variability in response to ligand binding. Furthermore, the reduction of the transition rate  $k_0$  of the core segment by several orders of magnitude suggests that this structural region of β<sub>2</sub>AR increases lifetime by orders of magnitude in the presence of BI, THRX, adrenalin, or carazolol. The spring constant κ of the core segment [H3-C2-H4-E2-H5.1] is slightly reduced from 0.59 N/m (unliganded state) to 0.48 N/m (BI), 0.44 N/m (THRX), 0.49 N/m (adrenalin), and 0.39 N/m (carazolol). This reduction in  $\boldsymbol{\kappa}$  indicates that the core segment increases mechanical elasticity by ~10%-20%. Finally, ligand binding stabilized the β<sub>2</sub>AR core segment [H3-C2-H4-E2-H5.1] by increasing free energy  $\Delta G^{\ddagger}$  by 7.7  $k_BT$  (BI), 6.9  $k_BT$  (THRX), 3.2 k<sub>B</sub>T (adrenalin), and 7.6 k<sub>B</sub>T (carazolol), compared to unliganded β<sub>2</sub>AR. Thus, the high-affinity ligands BI, THRX, and carazolol increased the free energy stabilizing the core segment twice as much compared to the natural agonist adrenalin.

Structural and functional data suggest that the core segment [H3-C2-H4-E2-H5.1] is important for ligand binding and β<sub>2</sub>AR activation:

- (1) Several amino acid residues of transmembrane  $\alpha$  helices H3 and H5 are part of the ligand-binding pocket (Gether et al., 2002). For instance H3 and H5.1 establish polar interactions and hydrophobic contacts with BI (Rasmussen et al., 2011). Two residues of H3, D113 and V114, contribute to agonist binding (Rasmussen et al., 2011). Furthermore, S203 of H5.1 is crucial for agonist binding, as shown by mutagenesis studies by Liapakis et al. (2000).
- (2) Receptor activation by agonists involves disruption of the ionic lock, which links the cytoplasmic parts of  $\alpha$  helices H3 and H6 in the inactive state (Ballesteros et al., 2001).
- (3) The second intracellular loop C2 is important for the efficiency of G protein activation and contains a switch that enables G protein coupling (Wess, 1997).

In summary DFS detected that binding of agonists and the inverse agonist carazolol increases structural flexibility, energetic stability, and lifetime (kinetic stability) of the functionally important core segment [H3-C2-H4-E2-H5.1]. These altered properties of the core segment enable β<sub>2</sub>AR to adopt more conformations from which certain conformations are supposed to represent an active state.

The affinities of the agonists investigated range from a K<sub>D</sub> of 0.84 pM (BI) to a  $K_D$  of 3.68  $\mu M$  (adrenalin).  $K_D$  of THRX is ~1 nM. Each agonist changed the conformational variability, kinetic stability, energetic stability, and mechanical elasticity of the structural core segment [H3-C2-H4-E2-H5.1] differently. A systematic relation may be found between the kinetic stability of [H3-C2-H4-E2-H5.1], which increased with increasing affinity of the agonists that bound to  $\beta_2AR$ . However, it should be noted that binding of agonists alone is insufficient to stabilize β<sub>2</sub>AR in the active state (Kobilka, 2011). Even binding of full agonists cannot stabilize every β<sub>2</sub>AR in the active state (Yao et al., 2009). The reason for this apparent discrepancy is that although bound to a ligand, the probability of  $\beta_2ARs$  to adopt other



functional states lowers but does not approach zero (Kobilka and Deupi, 2007). Interestingly, the active state can be further stabilized through interactions with G proteins or camelid antibodies (nanobodies) that exhibit G protein-like behavior (Kobilka, 2011; Rasmussen et al., 2011). Characterizing such stable β<sub>2</sub>AR/G protein complexes using DFS may be useful to quantify the conformational variability, kinetic stability, energetic stability, and mechanical elasticity of the structural core segment [H3-C2-H4-E2-H5.1] in the fully active state.

# **The Inverse Agonist Carazolol Introduces Major** Modifications to $\beta_2AR$

Among all ligands tested, carazolol modulated the properties of most structural segments of β<sub>2</sub>AR. Besides changing the energetic, kinetic, and mechanical properties of the core segment [H3-C2-H4-E2-H5.1] such as observed for the agonists, carazolol significantly affected three other structural segments: [H1.2-C1], [H2.1], and [H6.2-E3-H7-H8] (Table 1). Carazolol widened the energy valley stabilizing [H1.2-C1], [H3-C2-H4-E2-H5.1], and [H6.2-E3-H7-H8] by 0.10-0.27 nm. This indicates that these segments enhanced their conformational variability. Furthermore, carazolol reduced the transition rate  $k_0$  and, thus, increased the lifetime of each of the four structural segments by up to six orders of magnitude. The free energy  $\Delta G^{\ddagger}$  of structural segments [H1.2-C1] and [H3-C2-H4-E2-H5.1] increased by  $\sim$ 10  $k_{\rm B}T$ . Carazolol slightly lowered the spring constants  $\kappa$ of structural segments [H2.1], [H3-C2-H4-E2-H5.1], and [H6.2-E3-H7-H8], thereby increasing their structural elasticity. The strongest effect was observed for the structural segment [H1.2-C1], where  $\kappa$  reduced from 2.02 N/m in the unliganded state to 0.83 N/m in the carazolol-bound state.

Several amino acid residues of α helices H3, H5, H6, and H7 are important for carazolol binding (Rosenbaum et al., 2007). For instance W109, V114, and V117 of  $\alpha$  helix H3 establish hydrophobic contacts with carazolol. Additionally, polar interactions between carazolol and D113 of  $\alpha$  helix H3 as well as S203 of H5.1 are crucial for carazolol binding. Furthermore, hydrophobic contacts between W286, F289, and F290 of  $\alpha$  helix H6 and carazolol contribute to binding of the inverse agonist (Cherezov et al., 2007; Rasmussen et al., 2007). Moreover, loop E2 of the structural segment [H3-C2-H4-E2-H5.1] establishes a salt bridge with extracellular loop E3 in the inactive state (Bokoch et al., 2010). Carazolol stabilizes packing interactions involving 1121 (H3), P211 (H5.1), F282 (H6.2), and N318 (H7) that contribute to a network of interactions that stabilize an inactive conformation of the receptor (Kobilka, 2011). Thus, from this point it may not be surprising that we detect that the structural segments [H3-C2-H4-E2-H5.1] and [H6.2-E3-H7-H8] change their properties upon carazolol binding. However, DFS quantifies to what extent the properties of these and other structural regions change.

# **Carazolol Modifies Structural Regions Proposed** to Be Involved in Oligomerization

Inverse agonists promote higher-order β<sub>2</sub>AR oligomerization that alters access to other signaling proteins (Fung et al., 2009). The significant changes of the energy barriers  $(x_u, k_0, \text{ and } \Delta G^{\ddagger})$  and spring constants (κ) characterizing the structural segments [H1.2-C1], [H3-C2-H4-E2-H5.1], and [H6.2-E3-H7-H8] in the presence of carazolol are of particular interest because they significantly increase conformational variability, mechanical flexibility, kinetic stability, and energetic stability upon carazolol binding. It has been proposed for several other class A GPCRs that oligomerization involves primarily the interface between  $\alpha$  helices H1 and H8 (Guo et al., 2008; Liang et al., 2003). Thus, all structural segments changing their properties may contribute to the oligomerization of  $\beta_2$ AR. Particularly  $\alpha$  helices H4 and H5 are involved in the native packing arrangement of rhodopsin and define the rhodopsin dimer (Liang et al., 2003). It is therefore likely that the increased conformational variability of the core segment [H3-C2-H4-E2-H5.1] contributes to the formation of dimers and higher-ordered oligomers in the presence of carazolol. Conversely, interactions between protomers changing their oligomeric state can influence the parameters quantified by DFS (Sapra et al., 2006a). Thus, we cannot distinguish whether changes of the structural segments are induced by carazolol binding or carazolol-induced oligomerization.

## **Carazolol Employs Direct and Indirect Interactions** to Modify Structural Regions

Although carazolol binds to β<sub>2</sub>AR with picomolar affinity (comparable to BI), it significantly changed the energy landscape of four structural segments. The effect of carazolol on the energy landscape of the receptor is more pronounced compared to the effects caused by any of the other agonists or the neutral antagonist investigated. Not all of the structural segments are supposed to interact directly with carazolol (Rosenbaum et al., 2007). Thus, we conclude that carazolol binding changes the properties of the structural regions of β<sub>2</sub>AR by direct interactions and by indirect interactions, which do not result from directly contacting the ligand.

### **Conclusions**

Energy landscapes describe conformational variability, kinetic stability, energetic stability, and mechanical elasticity of proteins (Janovjak et al., 2008). GPCRs adopt many different conformations that are closely related to functional states (Kobilka and Deupi, 2007). Our work contributes to a more detailed understanding of the energetic, kinetic, and mechanical properties of native-like β<sub>2</sub>ARs reconstituted into membranes of phospholipids and cholesterol. We observed that the interactions of unliganded β<sub>2</sub>AR stabilize well-defined structural segments of the receptor. In the presence of a ligand, SMFS could not detect drastic changes of these interactions, and the stabilizing structural segments did not change positions. Thus, it can be concluded that ligand binding to  $\beta_2AR$  induces rather weak interactions instead of strong localized interactions. However, DFS showed that the interactions established upon ligand binding were sufficient to change the conformational, energetic, kinetic, and mechanical properties of structural segments of  $\beta_2AR$ .

Agonist or inverse agonist binding increased the conformational variability, kinetic stability, energetic stability, and mechanical elasticity of the functionally important structural core segment [H3-C2-H4-E2-H5.1] of β<sub>2</sub>AR. To what extent individual ligands could change the properties of the core segment was intrinsic to the ligand. In contrast to the agonists (BI, THRX, and adrenalin), the inverse agonist carazolol affected, in addition to the core segment, three structural segments: [H1.2-C1],



[H2.1], and [H6.2-E3-H7-H8]. Finally, the neutral antagonist alprenolol changed only the properties of structural segment [H1.1]. The functionally important structural core segment of the receptor remained unaffected by alprenolol.

Taken together, our single-molecule experiments reveal that ligands establish interactions that modulate the properties of distinct structural segments within  $\beta_2 AR$ . Quantifying the energetic, kinetic, and mechanical parameters of the structural segments provides insight into how these structural segments stabilize ligand-specific conformations of the receptor. Depending on which structural segments change their energetic, kinetic, or mechanical properties, the receptor samples more active states in the presence of agonists or more inactive states in the presence of the inverse agonist.

#### **EXPERIMENTAL PROCEDURES**

#### Cloning, Purification, Overexpression, and Reconstitution of $\beta_2AR$

Sf9 insect cells were grown at 27°C in suspension cultures in ESF-921 medium (Expression Systems, USA) supplemented with 0.5 mg/ml gentamicin. The Bac-to-Bac Baculovirus Expression System (Invitrogen, USA) was used for generating baculovirus for the  $\beta_2 AR$ . We used a modified construct of human β<sub>2</sub>AR with a truncated C-terminal end (48 aa) and a N-terminal FLAG epitope followed by a TEV protease cleavage site (Figure 2). β<sub>2</sub>AR expression was accomplished by infecting Sf9 cells at a density of  ${\sim}3~\times~10^6$  cells/ml for ~48 hr. Cells expressing receptors, as assessed by immunofluorescence, were harvested by centrifugation (15 min at 5,000  $\times$  g). Cell pellets were stored at  $-80^{\circ}$ C. From these pellets  $\beta_2AR$  was purified using a three-step purification procedure as described by Fung et al. (2009). For preparation of lipids, 1,2-dioleoyl-sn-glycero-3-phosphocholine (DOPC) (Avanti Polar Lipids, USA) and the cholesterol analog CHS (Steraloids, USA) were mixed and dissolved in chloroform to form a stock solution of lipids at concentrations of 20 and 10 mg/ml. DOPC and CHS were added to a glass vial, with DOPC at a 10-fold excess, and the chloroform was evaporated under a fine stream of argon. The lipids were then dried under vacuum for 1 hr. After this, the lipids were resuspended in 100 mM NaCl, 1% (w/v) octylclucoside, 20 mM HEPES (pH 7.5), vortexed, and sonicated for 1 hr in an ice water bath. The lipid mixture was stored at  $-80^{\circ}$  C.  $\beta_2$ AR was reconstituted as described previously by Fung et al. (2009). Briefly, 300 µl samples were prepared containing lipid and the β<sub>2</sub>AR at a lipid-to-receptor ratio of 1,000:1 (mol:mol). The lipid/receptor mixture was mixed with reconstitution buffer (100 mM NaCl. 20 mM HEPES [pH 7.5]) at a final volume of 300 μl and placed on ice for 2 hr. Vesicles were formed removing detergent on a Sephadex G-50 (fine) column (25 × 0.8 cm) using reconstitution buffer. To bind ligands,  $\beta_2 \text{AR}$  was preincubated for 1 hr at room temperature ( $\sim$ 22°C) with saturating amounts of ligand: 10  $\mu M$  for BI, THRX, and carazolol, 100  $\mu M$  for alprenolol, and 100  $\mu M$  for adrenalin. During subsequent reconstitution steps the same concentration of ligand was included in the reconstitution buffer.

### SMFS and DFS

SMFS was conducted using two different AFMs that provided similar results: ForceRobot 300 (JPK Instruments, Germany) and Nanoscope IIIa PicoForce AFM (Bruker, Germany). SMFS data of β<sub>2</sub>AR were recorded at pulling velocities of 100, 300, 600, 900, 1,200, 2,500, and 5,000 nm/s. SMFS at pulling velocity of 5,000 nm/s was recorded using a 16 bit data acquisition hardware (Nanoscope IIIa: NI PCI-6221; ForceRobot 300: NI PCI-6251, National Instruments, Germany). Cantilevers used (60  $\mu m$  long silicon nitride A-BioLever, BL-RC150 VB, Olympus, Japan) had nominal resonance frequencies of ~8 kHz in water. Cantilever spring constants (~30 pN/nm) were determined in buffer solution using the equipartition theorem by Butt and Jaschke (1995) prior to experiments. Due to uncertainties in calibrating the cantilever spring constant (~10%), β<sub>2</sub>AR was unfolded using at least five different cantilevers for each velocity. Proteoliposomes containing  $\beta_2AR$  were adsorbed over night at 4°C onto freshly cleaved mica in SMFS buffer (300 mM NaCl, 25 mM MgCl<sub>2</sub>, 25 mM Tris [pH 7.0]). Mica is an atomically flat, chemically inert, and hydrophilic surface that, so far, did not significantly influence the structure-function

relationship of membrane proteins and their interactions probed by SMFS (Müller and Engel, 2007). To remove weakly attached membrane patches, the sample was rinsed several times with SMFS buffer. SMFS buffer solutions were prepared using nanopure water (18 MOhm/cm; PURE-LAB Ultras, ELGA LabWater) and pro-analysis grade chemicals from Sigma-Aldrich or Merck. To characterize ligand binding, SMFS buffer was supplemented with adequate amounts of the ligand. Unfolding events were monitored recording the cantilever deflection and the distance separating cantilever stylus and membrane. Interaction forces were calculated from the cantilever deflection using Hook's law.

#### **Data Selection**

Mechanical unfolding of β<sub>2</sub>AR was recorded by F-D curves. Each force peak of a F-D curve denoted the rupture of an unfolding barrier established by a structural segment of  $\beta_2AR$ . The distance at which a force peak was detected assigned the contour length of the unfolded and stretched polypeptide that tethered the AFM stylus and the anchoring structural segment. The very last force peak of a F-D curve represented the unfolding of the last structural segment remaining anchored by the membrane bilayer (Müller et al., 2002), Overcoming the stability of this last segment led to complete unfolding of the receptor, followed by extraction from the membrane. In the GPCR bovine rhodopsin, the last structural segment (or unfolding barrier) corresponds to helix H8, which lies parallel to the membrane bilayer followed by a palmitoylation site (Sapra et al., 2006b). We assumed that this was also the case for β<sub>2</sub>AR because it shares very similar structural features with rhodopsin. A fully stretched  $\beta_2 AR$ polypeptide that remains anchored by helix H8 would show a contour length of  $\sim\!\!260$  to 290 aa. Therefore, F-D curves showing a maximum length of 70-90 nm (~260-290 aa) were selected for data analysis.

#### **Data Analysis**

Every force peak of a F-D curve was fitted using the WLC model by Bustamante et al. (1994):

$$F(x) = \frac{k_{\rm B}T}{P} \left[ 0.25 \left( 1 - \frac{x}{L} \right)^{-2} - 0.25 + \frac{x}{L} \right].$$
 (Equation 1)

A persistence length (P) of 0.4 nm and a backbone length of 0.36 nm were assumed for every amino acid. The contour length (L) (in amino acids) obtained from fitting a force peak using the WLC model describes the length of the polypeptide that had been unfolded and stretched. Contour lengths and rupture forces were statistically analyzed for every reproducibly occurring force peak using built-in and custom procedures of IgorPro 6 (WaveMetrics, USA). To superimpose F-D curves, they were aligned at the characteristic force peak detected at a contour length of 121 aa.

#### **Assignment of Stable Structural Segments**

The contour length determined by WLC fitting corresponds to the length of the unfolded and stretched  $\beta_2AR$  polypeptide that tethers AFM stylus and a structural unfolding intermediate. Thus, every force peak could be used to assign the end of the previous and the beginning of the following structural segment that stabilized  $\beta_2AR$  against unfolding (Kedrov et al., 2007a). Some stable structural segments had to be assumed to begin at the cytoplasmic  $\beta_2AR$  surface at the opposite side of the pulling AFM stylus. To locate the beginning of such a stable structural segment, the thickness of the membrane ( $\sim\!4$  nm) was added to the contour length of the corresponding force peak (Kedrov et al., 2007a). Accordingly,  $\sim\!11$  aa (11 aa  $\times$  0.36 nm/aa) was added to the contour length of a force peak. If the beginning of a stable structural segment was located within the membrane, less amino acids were added to the contour length.

### Calculation of $\boldsymbol{x}_u$ and $\boldsymbol{k}_0$

The Bell-Evans theory by Evans (1998) describes the most probable unfolding force  $(F^*)$  as a function of the most probable loading rate  $(r_1^*)$  to reveal insight into the unfolding energy barrier that stabilizes a structural segment against unfolding (Evans and Ritchie, 1997). The relation between  $F^*$  and  $r_f^*$  can be described by:

$$F^* = \frac{k_B T}{x_u} \ln \left( \frac{x_u r_f^*}{k_B T k_0} \right).$$
 (Equation 2)



 $k_{\rm B}$  is the Boltzmann constant, T the absolute temperature,  $r_{\rm f}^{\star}$  the most probable loading rate,  $x_{\rm u}$  the distance between the free energy minimum and the transition state, and  $k_0$  the unfolding rate at zero applied force. Using a nonlinear least-squares algorithm, the parameters  $x_u$  and  $k_0$  were obtained by fitting Equation 1 to a DFS plot (Figure 4). The loading rate was calculated using  $r_f = k_{\text{spacer}} v$ , where  $k_{\text{spacer}}$  is the spring constant of the stretched polypeptide and v the pulling velocity.  $k_{\rm spacer}$  corresponds to the slope of a force peak before rupture. Experimental force and loading rate histograms were fitted using Gaussian distributions.

#### **Calculation of Transition Barrier Height and Mechanical Spring** Constant

The free energy barrier  $\Delta G^{\ddagger}$  separating the unfolded from the folded state was calculated using the Arrhenius equation:

$$\Delta G^{\ddagger} = -k_{\rm B}T \ln (\tau_{\rm D}k_0). \tag{Equation 3}$$

 $\tau_{\text{D}}$  is the diffuse relaxation time (Dietz and Rief, 2004) and is typically in a range between  $10^{-7}$  and  $10^{-9}\ s$  (Krieger et al., 2003). We used a  $\tau_D$  of  $10^{-8}\ s$  in our calculations. Varying  $\tau_D$  in the aforementioned range would change  $\Delta G^{\ddagger}$  by <15%. Furthermore, the influence of errors of  $\tau_D$  would be the same for all conditions and  $\Delta G^{\ddagger}$  values, even if  $\tau_D$  was wrong by orders of magnitude. Errors in  $\Delta G^{\ddagger}$  were calculated by propagation of errors of  $k_0$ . Without having information on the energy potential shape, we assumed a simple parabolic potential and calculated the mechanical spring constant  $\kappa$  of a structural segment using  $\Delta G^{\ddagger}$  and  $x_u$  (Dietz et al., 2006) with the following equation:

$$\kappa = \frac{2 \Delta G^{\ddagger}}{X_{ii}^2}.$$
 (Equation 4)

To estimate errors in  $\kappa$ , errors in  $\Delta G^{\ddagger}$  and  $x_{\mu}$  were propagated.

## SUPPLEMENTAL INFORMATION

Supplemental Information includes five figures and three tables and can be found with this article online at doi:10.1016/j.str.2012.05.010.

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