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ORIGINAL PAPER

# Measurement of Reactive Hydroxyl Radical Species Inside the Biosolutions During Non-thermal Atmospheric Pressure Plasma Jet Bombardment onto the Solution

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**Abstract** Non-thermal atmospheric pressure plasma jet could generate various kinds of radicals on biosolution surfaces as well as inside the biosolutions. The electron temperature and ion density for this non-thermal plasma jet have been measured to be about  $0.8\sim 1.0$  eV and  $1 \times 10^{13} \text{ cm}^{-3}$  in this experiment, respectively, by atmospheric pressure collisional radiative model and ion collector current. In this context, the hydroxyl OH radical density inside the biosolutions has been also investigated experimentally by ultraviolet absorption spectroscopy when the Ar non-thermal plasma jet has been bombarded onto them. It is found that the emission and absorption profiles for the other reactive oxygen species such as NO (226 nm) and  $\text{O}_2^{*-}$  (245 nm) are shown to be very small inside the biosolution in comparison with those for the OH radical species. It is found that the densities of OH radical species inside the biosolutions are higher than those on the surface in this experiment. The densities of the OH radical species inside the deionized water, Dulbecco's modified eagle medium, and phosphate buffered saline are measured to be about  $2.1 \times 10^{16}$ ,  $1.1 \times 10^{16}$ , and  $1.0 \times 10^{16} \text{ cm}^{-3}$ , respectively, at 2 mm downstream from the surface under optimized Ar gas flow of 200 sccm. It is also found that the critical hydroxyl OH radical density for the lung cancer H460 cells to experience an apoptosis is observed to be around  $0.3 \times 10^{16} \text{ cm}^{-3}$  under 1 min plasma exposure in this experiment.

**Keywords** Non-thermal atmospheric pressure plasma jet · Atmospheric pressure collisional radiative model · Hydroxyl OH radical density inside the biosolution · Ultraviolet absorption spectroscopy

## Introduction

For elimination of the limitations for vacuum plasma operation with least amount of energy and cost, so-called non-thermal atmospheric pressure plasma jet (hereafter non-thermal

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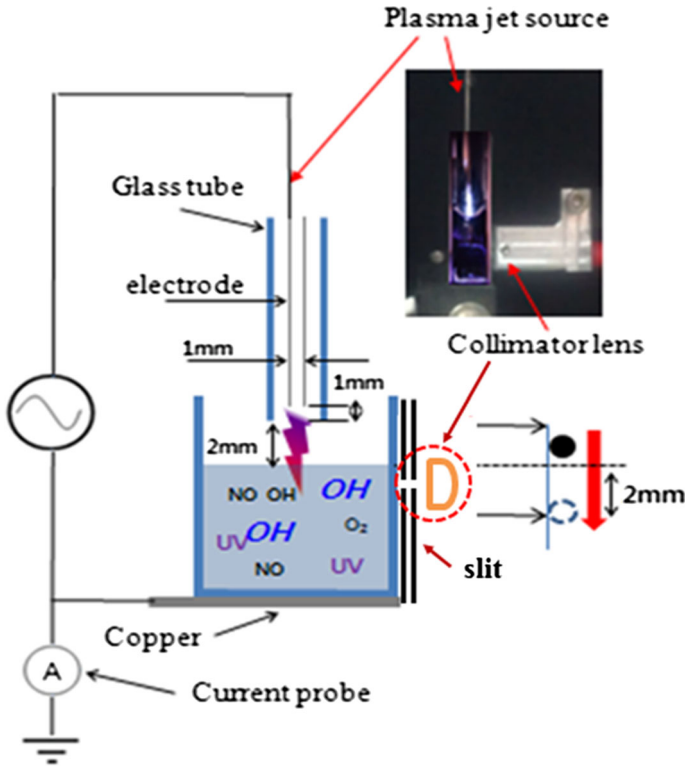
plasma) has been emerged recently. Also, this kind of non-thermal plasma has been attracted to areas of biotechnology with their diversity of forms for easy use. Especially, a lot of various reactive chemical species could be generated by non-thermal plasma jet. Non-thermal plasmas jets with diverse types have recently been developed and used in emerging novel biomedical applications. Besides its sterilization effects, the first practical studies on plasma-based treatment of chronic wounds or tumor treatment with non-thermal plasma jet has been very promising [1–4]. There are many plasma jets using various electrode configurations. The direct plasma jets with other types of electrodes are widely used for biomedical [5–9], in which the plasma jets with a needle electrode are one of them. For achievements of the technical requirements for medical instrumentation, advanced non-thermal plasma sources must have some electron temperature and requires specified radical species.

Chemically reactive oxygen species (ROS) and reactive nitrogen species (RNS) play an important role in biomedical field during non-thermal plasma treatment. These effects of ROS and RNS on the biological cells are not studied well yet. Based on these situations, the convergence technology of plasma and biology is highly developed and its research range is widely expanded. Of these species, hydroxyl radical OH, hydrogen peroxide  $H_2O_2$  as well as nitric oxide NO species could be generated by non-thermal plasma jet, which is operating at the atmospheric pressure when it contacts with the biosolution surface. Moreover, the non-thermal plasma interaction with biosolutions has received increasing attention for their biomedical applications. It is very important to measure the hydroxyl radical OH density by using the ultraviolet absorption spectroscopy on the biosolutions [10] as well as inside them induced by the non-thermal plasma jet.

Nowadays, the convergent studies of the non-thermal plasma and biomedicines have been actively increased with high research extension and speed. The ROS radicals generated inside the biosolutions are not sufficiently investigated during non-thermal plasma interactions with bio-solutions. Also the basic mechanisms for the ROS generation inside the biosolution are not well known yet during non-thermal plasma bombardment onto the biosolution surface. Therefore, in this paper, we investigate the hydroxyl OH radical density inside the biosolutions during the non-thermal plasma bombardment on the biosolution surface by ultraviolet absorption spectroscopy as well as electron temperature and density characteristics for argon non-thermal plasma jet by atmospheric pressure collisional radiative spectroscopy [11].

## Experimental Procedure

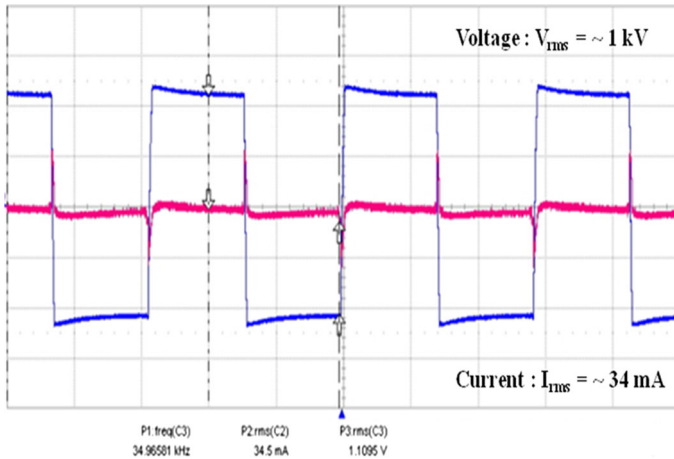
Figure 1 shows the schematic experimental setup for the needle-typed non-thermal plasma jet operating at the atmospheric pressure, which is bombarding onto the biosolution surface. We have used an argon gas flow in this experiment for the generation of non-thermal plasma jet. Our non-thermal plasma jet consists of needle-type powered electrode whose diameter is 1 mm, which is located by 1 mm upward from the end of the cylindrical glass tube, whose diameter is 5 mm in diameter. Grounded electrode is located by 13 mm away from the end of glass tube tip, which is the rear bottom surface of quartz, in which the water is filled. The distance between the powered electrode and water surface is set by 3 mm. For Ar gas flow rates ranged from 100 to 350 sccm, the electron temperature and plasma ion density of non-thermal plasma jet have also been measured by optical emission spectroscopy based on the atmospheric pressure collisional radiative (CR) model [12] and by the electrical ion current signals at the grounded collector electrode passing through the



**Fig. 1** Schematic experimental setup for the plasma generation for the needle-typed non-thermal argon plasma jet operating at the atmospheric pressure

floating mesh during the non-thermal plasma jet bombardment onto biosolutions. We have investigated the optical emission spectrum emitted from four 2p metastable Ar emission lines of 696.5, 706.7, 922.4, and 912.3 nm for the measurement of electron temperature based on the atmospheric pressure CR model [11]. The two electrodes in a non-thermal plasma jet have been connected to a square-pulse power supply. Figure 2 shows the voltage and current waveforms applied to the non-thermal plasma jet. It is shown that the voltage signal,  $v$ , has a root-mean-square voltage of about 1 kV and peak current,  $I$ , of 34 mA, with current duration of about 2.1  $\mu$ s, where the electrical power is given by about 4.9 W, which is obtained from  $\frac{1}{T} \int_0^T iv dt$ , where T is period of squared pulse with the repetition rate of about 35 kHz.

For measurement of hydroxyl OH radical density, the non-thermal plasma jet has been in contact with the biosolution surface and its optical emission signal has been observed by charge-coupled device (CCD) spectrometer connected by the double slit and optical fiber with collimator lens. Also we have measured the reactive oxygen species, especially, for the hydroxyl OH radicals by the optical emission spectroscopy as well as its absolute density inside the biosolutions by the ultraviolet (UV) absorption spectroscopy when the non-thermal plasma has been bombarded onto the biosolution surface. Figure 3 shows the schematic experimental setup for the ultraviolet absorption spectroscopy inside the biosolutions. This system consists of deuterium UV lamp in this experiment, whose power is 30 W with spectral wavelength between 160 and 800 nm, plano-convex lens whose



**Fig. 2** Electrical voltage and current signals applied to the non-thermal Ar plasma jet

transmission wavelength ranges are from ultraviolet to infrared, double slit connected to the collimator lens, and CCD spectrometer with optical fiber whose spectral range is from 200 to 1,100 nm. The light of UV lamp has been incident and focused by 3 mm plano-convex lens in front of detector system for the measurement of absorption profiles occurred at 309 nm, of the hydroxyl radical OH species [4, 12], as shown in the Fig. 3. This detector system consists of double slit in this experiment, whose slit width is 100  $\mu\text{m}$  and their gap is 1 mm, and then collimator lens have been connected to the optical fiber whose diameter is 500  $\mu\text{m}$ . With this experimental situation, we observed no stray light from above the surface since the plasma jet has been bombarded onto the central surface region in the measurement.

The hydroxyl OH radical density inside the biosolution, which is generated by the argon non-thermal plasma jet interaction with DI water surface, could be obtained by ultraviolet absorption spectroscopy using the Lambert–Beer’s law [4]. The incident UV light on the biosolution has the intensity  $I_o$  and the transmitted light intensity is denoted by  $I_v$  after passing through the OH existing region inside quartz tube ( $x = 10$  mm), in which the hydroxyl OH radical species are generated by the non-thermal plasma bombardment onto the solution surface. The density of hydroxyl radical species, OH, inside the biosolution, which is induced by the non-thermal plasma bombardment onto the biosolution is given by [4]

$$N = -\frac{1}{\sigma \cdot x} \ln\left(\frac{I_v}{I_o}\right), \quad (1)$$

where  $N$  is the density or concentration for absorbing species of hydroxyl OH radicals,  $\sigma$  is the cross sectional area of about  $1.2 \times 10^{-16}$   $\text{cm}^2$  for absorbing species of hydroxyl radical OH species [4]. The hydroxyl radical OH density inside the biosolution could be obtained in Eq. (1), by measurement of the ratio  $I_v/I_o$  of the transmitted intensity to the incident one during non-thermal plasma irradiation onto the biosolution. Here the optimized gas flow condition has been also investigated for maximizing the density of hydroxyl OH radical

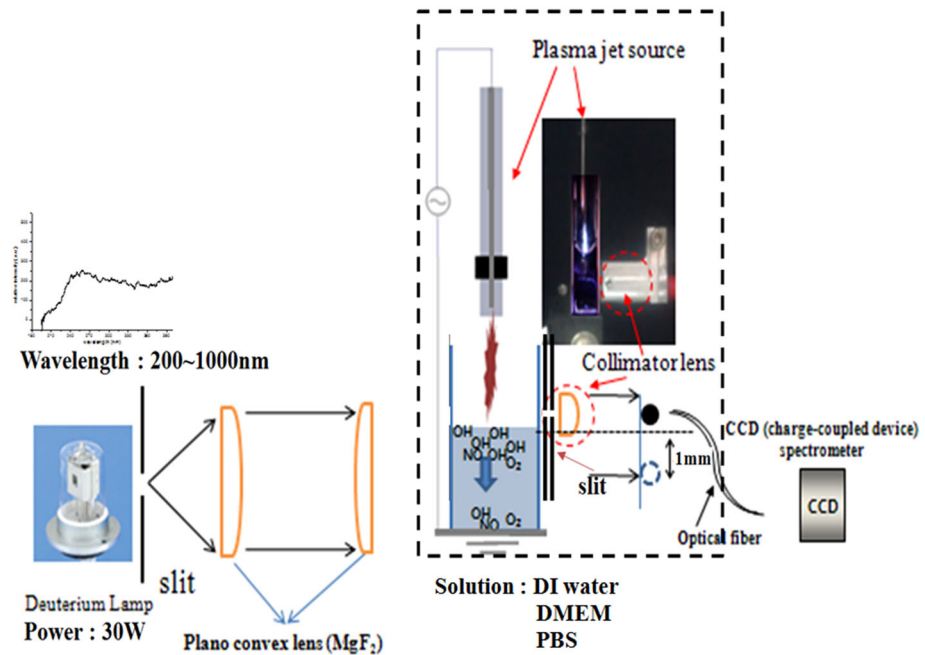


Fig. 3 Schematic experimental setup of ultraviolet absorption spectroscopy below the biosolutions

species inside the biosolution under the argon non-thermal plasma jet bombardment onto the solution.

### Results and Discussion

#### Electron Temperature and Ion Density Measurement of Argon Non-thermal Plasma Jet

Rare gases such like argon are very general plasma constituents in many applications. Especially, argon can provide useful diagnostics such as electron temperature of non-thermal plasma operating at atmospheric pressure. CR model might be performed for pure Ar gas as long as possible. We have tried to apply the CR model for Ar plasma in contact with biological solution where there are very large amount of water vapor and the plasma-forming gas, since the excited 2p emission lines from Ar atoms are not changed by addition of water molecules and other plasma-forming gases. The electron temperature in Ar plasma in contact with biological solution could be measured accurately by our CR model, since the physical parameters of rate coefficients for Ar gas plasma have been well studied and established [13] for electron temperature measurements. We have also assumed that these physical parameters of rate coefficients for Ar gas at atmospheric pressure can be used even to the environments in contact with biological solutions. Therefore, the CR model for Ar plasma in contact with biological solution could be used for the measurement of electron temperature as in pure Ar gas without any loss of generality.

A simple atmospheric pressure CR model can be used to determine the electron temperature of non-thermal plasma even operating at atmospheric pressure by using the relative emission intensities of only four argon lines [11]. In this method, a Maxwell–Boltzmann distribution for the electron energy distribution function (EEDF) for the non-thermal plasma jet is assumed, and experimental metastable emission data are utilized so that an electron temperature could be obtained. The atmospheric pressure CR model is based on the balance equation of the four excited level densities from any of the 2p levels. Population of the 2p excited argon levels ( $2p_1 \sim 2p_{10}$  in Paschen notation) mainly occurs by electron collisions with argon atoms in the ground level and with atoms in the metastable levels ( $1s_3$  and  $1s_5$  in Paschen notation) [11]. Here the excited Ar atoms to 2p levels from resonant states ( $1s_2$  and  $1s_4$ ) and quenching effects caused by the excited atoms from higher 3p levels [13] have been neglected for analytical simplicity since most of emission intensities are caused by electron impact in this experiment. Therefore, the balance equation for a  $2p_x$  (Paschen notation) excited level can be written as,

$$n_e n_g k_{g,2p_x} + \sum_{i=3,5} n_e n_{1s_i} k_{1s_i,2p_x} = \sum_{i=5}^2 n_{2p_x} A_{2p_x,1s_i}, \quad (2)$$

where  $n$  indicates number density ( $n_e$ : electron density,  $n_g$ : neutral gas density,  $n_{1s_i}$ : 1 s level number density,  $n_{2p_x}$ : 2p level number density),  $k_{x,y}$  is the rate coefficient for the excitation from level  $x$  to  $y$ , and  $A_{y,x}$  is the transition probability form level  $y$  to  $x$ . The subscript  $g$  stands for ground level,  $e$  for electrons, and  $1s_x$  and  $2p_x$  are the Paschen notations [11]. In Eq. (2), the rate coefficients  $k$  can be calculated according to the following

$$k(T_e) = \int_0^{\infty} \sigma(\varepsilon) \sqrt{\frac{2\varepsilon}{m}} f(\varepsilon, T_e) d\varepsilon, \quad (3)$$

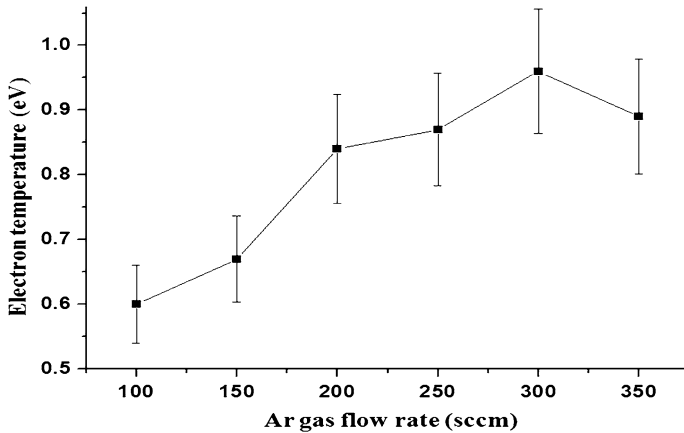
where  $\varepsilon$  is the energy,  $m$  is the electron mass,  $f$  is the Maxwell–Boltzmann EEDF,  $\sigma$  is the cross section of the collision between electrons and the particles [11]. The relative number density for specified wavelength was represented by the emission intensities observed to the spectrometer. For the reason, the  $n_x$  ( $x = 1s, 2p$ ) in Eq. (3) can be written as,

$$n_x \approx \frac{I_{x,y} \lambda_{x,y}}{A_{x,y}}, \quad (4)$$

where  $x$  and  $y$  represent upper and lower energy levels,  $I$  is the relative intensity, and  $\lambda$  the specified wavelength [11]. Eq. (4) can be used in Eq. (2) to replace  $n_{2p_x}$  and Eq. (2) can be written as follows

$$n_e = \frac{\sum_{i=5}^2 n_{2p_x} A_{2p_x,1s_i}}{n_g k_{g,2p_x} + \sum_{i=3,5} n_{1s_i} k_{1s_i,2p_x}} \quad (5)$$

This equation can be represented by any  $2p_x$  level (indicated as  $2p_2, 2p_3, 2p_6$  and  $2p_{10}$ ). It is noted here that these 2p metastable Ar emission lines are 696.5 nm ( $2p_2 \rightarrow 1s_5$ ), 706.7 nm ( $2p_3 \rightarrow 1s_5$ ), 922.4 nm ( $2p_6 \rightarrow 1s_2$ ), and 912.3 nm ( $2p_{10} \rightarrow 1s_5$ ). This electron density  $n_e$  is the same for four  $2p_x$  levels. Therefore, we can couple these equations as followings [11],



**Fig. 4** Electron temperatures of Ar non-thermal plasma jet at 2 mm above the biosolution versus the argon flow rates

$$\frac{\sum_{i=5}^2 n_{2p_a} A_{2p_a,1s_i}}{n_g k_{g,2p_a} + \sum_{i=3,5} n_{1s_i} k_{1s_i,2p_a}} = \frac{\sum_{i=5}^2 n_{2p_b} A_{2p_b,1s_i}}{n_g k_{g,2p_b} + \sum_{i=3,5} n_{1s_i} k_{1s_i,2p_b}} \tag{6}$$

$$\frac{\sum_{i=5}^2 n_{2p_c} A_{2p_c,1s_i}}{n_g k_{g,2p_c} + \sum_{i=3,5} n_{1s_i} k_{1s_i,2p_c}} = \frac{\sum_{i=5}^2 n_{2p_d} A_{2p_d,1s_i}}{n_g k_{g,2p_d} + \sum_{i=3,5} n_{1s_i} k_{1s_i,2p_d}} \tag{7}$$

The electron temperature  $T_e$  of any range value is replaced by  $k$  and Eqs. (6) and (7) can be solved with respect to metastable number densities  $n_{1s_3}$  and  $n_{1s_5}$ . For example, we can obtain two equations for the electron density  $n_{e-a}(T_e)$  of  $2p_a$  excited level and  $n_{e-c}(T_e)$  of  $2p_c$  excited level that are dependent on the electron temperature  $T_e$ . For obtaining the electron temperature of plasma jet, we have to find the specific electron temperature being satisfied with the condition,

$$n_{e-a}(T_e) = n_{e-c}(T_e) \tag{8}$$

This calculation process for obtaining the electron temperature can be easily processed using simple Matlab programming. The electron temperature for the argon non-thermal plasma jet operating at the atmospheric pressure with low electrical power of 4.9 W and driving frequency of 35 kHz could be measured by optical emission spectroscopy under the various Ar gas flows ranged from 100 to 350 sccm based on the atmospheric pressure CR model.

Figure 4 shows the measured electron temperatures for the argon non-thermal plasma jet versus the gas flow rates ranged from 100 to 350 sccm, obtained by the atmospheric pressure CR model with the four 2p metastable Ar emission lines. It is noted that these electron temperatures  $kTe$  have been measured at the region of 2 mm above the biosolution surface. It is found that electron temperature  $kTe$  has been increased up to about 1 eV as the argon gas flow rate is increased to 300 sccm, and it is slowly decreased beyond 300 sccm and reached to 0.9 eV at 350 sccm. It is noted that the propagating speed,  $v_p$ , of plasma jet is given by  $v_p = v^2/u_n$  [14] based on the diffusion wave-packet model, where  $v$  is the ion sound or Bohm’s velocity and  $u_n$  is density gradient gas speed. Here it is noted that  $v_p$  could be estimated as  $\sim 20$  km/s with  $u_n$  of  $\sim 10$  m/s [15], so that

the  $v$  is estimated to be  $0.4 \times 10^3$  m/s. From the equation of  $v \approx \sqrt{\frac{kT_e}{M}}$ , where  $M$  is atomic mass of Ar ( $M = 6.63 \times 10^{-26}$  kg), the electron temperature  $kT_e$  could be also obtained by about 1 eV. This electron temperature obtained from the ion sound speed  $v$  and the plasma propagation speed  $v_p$  is in good agreement with that obtained by atmospheric pressure CR model. There are, of course, uncertainties surrounding the use of a CR model that considers only argon to analyse a plasma jet impinging on a solution. However, because the measurements were taken 2 mm above the substrate, and because the electron temperature obtained from the ion sound speed and plasma propagation speed was in agreement, we believe that the temperatures are reliable.

The plasma ion density  $n_i$  can be obtained from measurements of the plasma ion collector current  $I_i$ , after passing through the floating mesh, which can be measured by [16]

$$n_i(r) = \frac{I_i}{2\pi e v \sigma^2} \exp\left(-\frac{r^2}{2\sigma^2}\right), \quad (9)$$

where  $e$  is electron charge,  $v$  is ion sound velocity,  $\sigma$  is the width of the Gaussian profile for emission intensity distribution of plasma jet, which is 6 mm in this plasma jet, and  $r$  is the radial distance from the center. The ion density has been measured by RMS value of ion current at the radial distance of  $r = 0$  in this experiment. At gas flow ranges between 150 and 300 sccm, the ion densities are measured to be about  $1 \times 10^{13}$  cm<sup>-3</sup>.

#### Optical Emission Spectroscopy of Non-thermal Plasma Jet Inside the Deionised (DI) Water

Especially, optical emission spectroscopy (OES) inside biosolutions is extremely useful for non-thermal plasma jet bombarding onto the surface since the information's for induced ROS and their spatial distribution characteristics could be obtained from these data. Atmospheric pressure non-thermal plasma could generate various kinds of reactive oxygen species inside the biosolutions during their interactions on the surface. Plasma-induced ultraviolets have been generated by reactive species of nitric oxide (NO) [17, 18], superoxide anion ( $O_2^{\bullet-}$ ) [19], hydrogen peroxide ( $H_2O_2$ ) [20], and hydroxyls (OH) [4, 10, 18, 21–23] on boundary surface of plasma and biosolutions. These ultraviolets, whose wavelength ranged from 210 nm (6 eV) to 309 nm (4.2 eV), propagate into solutions below more than 2 mm to excite the water molecules and dissociate them to induce ROS generation inside the biosolution. This is a mechanism for the ROS generation inside the solution.

Figure 5 shows the visual confirmation of OH radical species generation inside the deionized (DI) water by bombardment of non-thermal plasma jet onto the water surface, in which vinyl filter has been placed just below the water surface, with (left hand side) and without (right hand side) inclusion of terephthalic acid (TA) [24]. The vinyl filter could pass only ultraviolet lights from 260 to 320 nm, however, the plasma particles are prohibited from this filter. It is found that the hydroxyl OH radical species could be generated inside the DI water since the color of the DI water including TA is changed to blue in this experiment. The water  $H_2O$  molecules could be excited to higher energy levels  $H_2O^*$  and dissociated into OH by these successive UV exposures to them, whose wavelengths are mainly 309 nm which are about 4 eV, i.e.,  $UV + H_2O \rightarrow H_2O^*$  and  $UV + H_2O^* \rightarrow OH + H$ . Hence we could think that the plasma-induced ultraviolet lights on the biosolution play a major role for production of reactive oxygen species inside the biosolutions by propagation into them.



**Fig. 5** Generation of OH radical species by non-thermal plasma in deionized (DI) water with inclusion of terephthalic acid (TA)

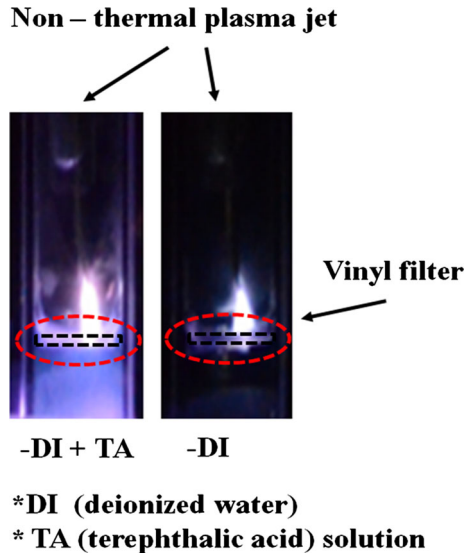
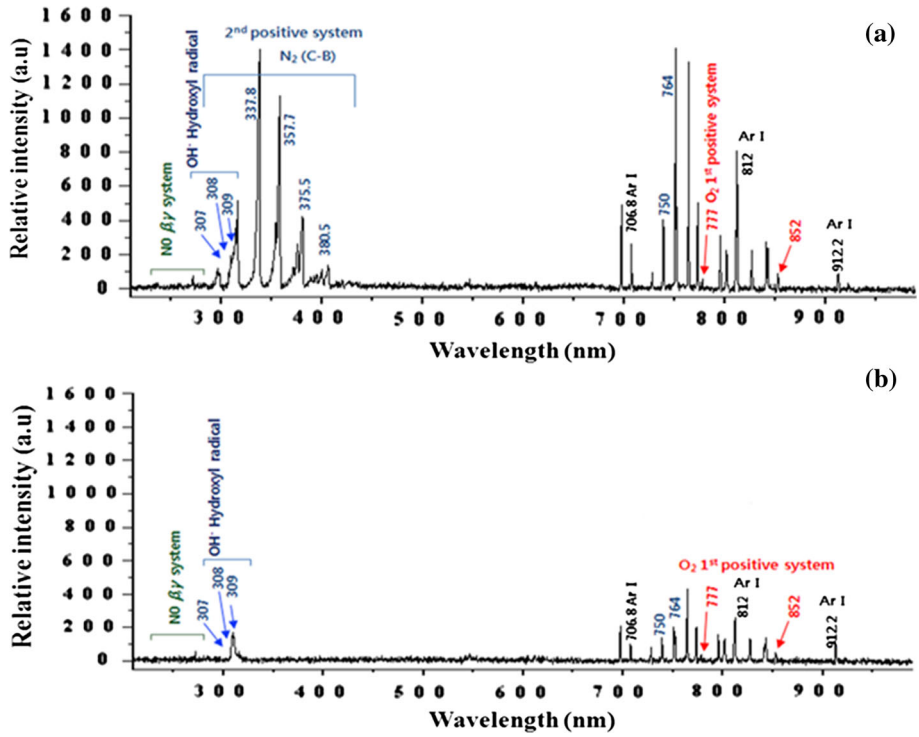


Figure 6 shows the optical emission spectrum measured by CCD spectrometer with optical fiber at the 2 mm above the deionised (DI) biosolution surface (a), and 2 mm below the the DI biosolution surface (b). From the result of spectrum of Fig. 6a, the Ar emission lines between 700 and 900 nm are shown to be dominantly appeared and it is found that the 309 nm emitted from the hydroxyl OH radical [4, 8, 18, 21–23] species, 224 nm from the nitric oxide NO [17, 18], the emission lines 245 nm from the reactive species of superoxide anion  $O_2^{*-}$  [19], and the emission lines from  $N_2$  second positive system ( $C3\Pi_u-B3\Pi_g$ ) ranged from 320 to 380 nm are strongly appeared just above the biosolution surface. While as seen in Fig. 6b, as moved 2 mm downward into the DI biosolution surface, the emission lines of 224~280 nm from the nitric oxide NO [17, 18], the 245 nm from the reactive species of superoxide anion  $O_2^{*-}$  [19] are shown to be decreased and disappeared. Also it is found that the 309 nm emitted from the hydroxyl OH radical species gets stronger in the biosolution than that above the solution. It is also noted from the Fig. 6a and b that the both lines of 777 and 852 nm inside the DI biosolution, which are emitted from the  $O_2$  first positive system, including the emission lines of Ar are getting weaker than those above the solution.

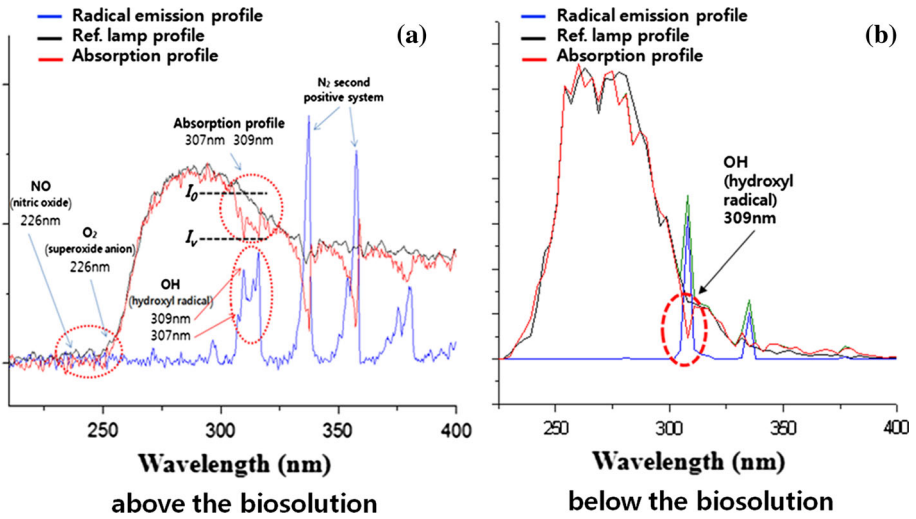
#### Density of Hydroxyl OH Radical Species and Its Influence on the Biological Cells

The density of the hydroxyl radical species has been investigated at the region of 2 mm above the interfacial solution surface [10], where the UV passing length is 3 mm, as well as inside the biosolution whose spatial passing length is 10 mm, by the ultraviolet absorption spectroscopy in Ar gas flow ranged from 100 to 350 sccm in argon non-thermal plasma jet. At this time the position of the deuterium lamp and plano-convex lens system have been fixed during the measurement. For the measurement of OH radical species at the different position inside the biosolution, the detector system could be moved down from 2 mm below water surface with spatial resolution of 1 mm.

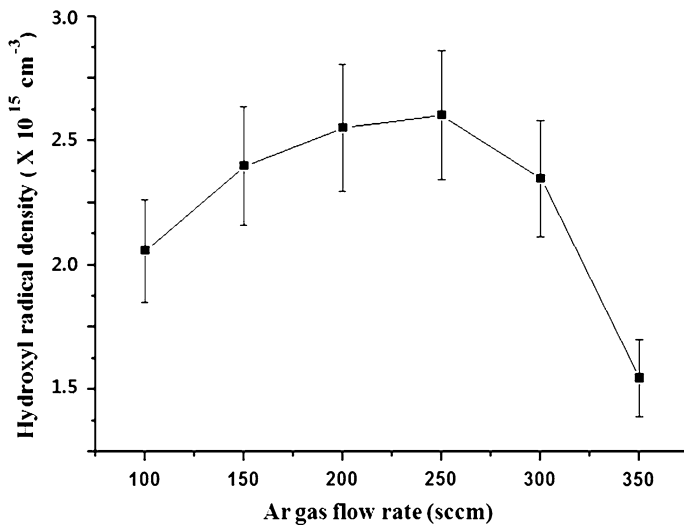


**Fig. 6** Optical emission spectrum measured by CCD spectrometer with optical fiber at 2 mm above DI water (a), and 2 mm below the DI water surface (b)

Figure 7 shows the UV emission and absorption spectral profiles caused by the OH radical species, at the region of 2 mm above the DI water surface (a) and inside them (b), respectively, versus the wavelengths. Also it is noted that reference UV lamp ( $I_0$ ) without non-thermal plasma has been shown at the upper line (black) and ROS emission profiles with non-thermal plasma have been shown at the bottom lines (blue), respectively, in Fig. 7a and b. It is especially noted that the OH absorption profiles are strongly appeared around the 306 ~ 309 nm at the round-dotted region (red) for both regions of Fig. 7a and b. It is also noted from Fig. 7 that the absorption profiles for the other ROS species such as NO (226 nm) and  $O_2^{*-}$  (245 nm) are shown to be very small above the DI surface of Fig. 6a, while they are disappeared inside the DI water of Fig. 7b. The absorption profiles of hydroxyl OH radical species (red) have been shown to be maximum in both Fig. 7a and b around the wavelength of 309 nm under the non-thermal plasma bombardment and the reference lamp is turned on. It is noted that the UV transmission ratio  $I_v$  to incident one  $I_0$  around 309 nm could be obtained by comparison between the emission profiles from the reference deuterium lamp (black) and the absorption profiles of OH radical species (red), as shown in the Fig. 7a. This transmission ratio ( $I_v/I_0$ ) for OH radical species has been measured to be 0.75 and 0.32, respectively, for on the surface and inside the biosolution, respectively, where the intensity reaches the maximum value in Fig. 7a and b. The emission and absorption spectra of OH in water are observed to be basically the same as those of OH in the gas phase, in this experiment, which are mainly occurred at 309 nm. We



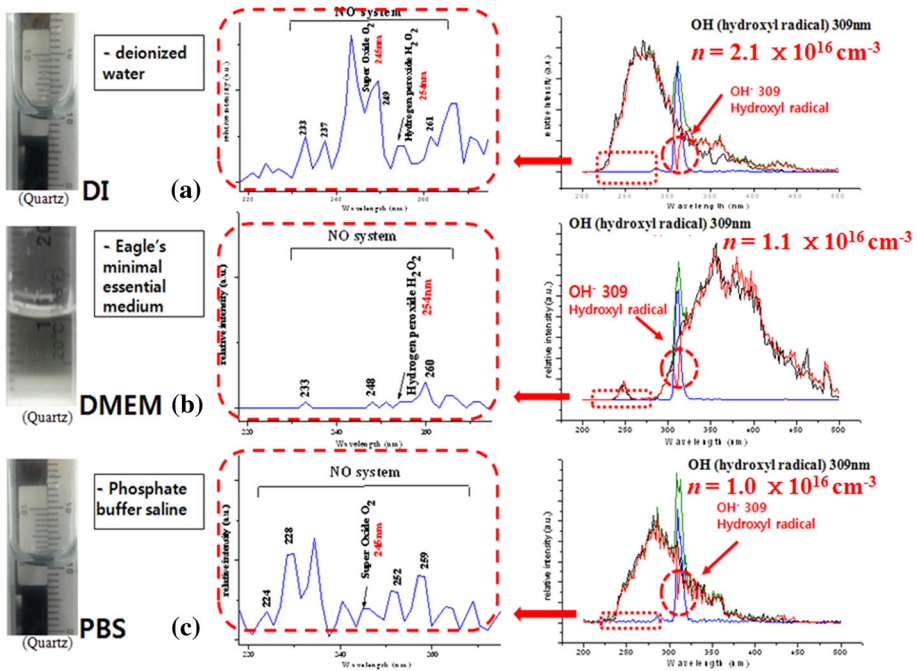
**Fig. 7** UV emission and absorption profiles caused by the ROS including OH species, above the deionized (DI) (a) and below it (b), versus the wavelengths



**Fig. 8** Density of hydroxyl OH radical species at the 2 mm above the deionized (DI) water surface, versus the Ar gas flow rates ranged from 100 sccm to 350 sccm

emphasize that we could measure OH density inside the biological solutions for OH region of  $x = 10$  mm using the UV absorption methods as in the gas phase above the DI water for OH region of  $x = 3$  mm.

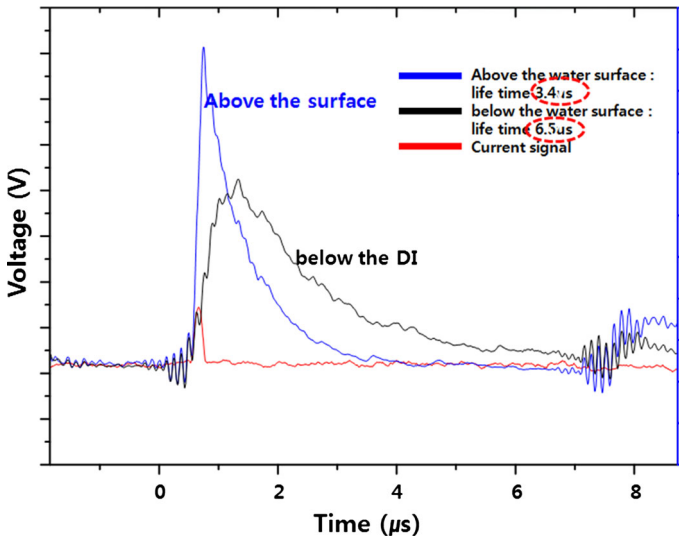
Figure 8 shows the density of hydroxyl OH radical species at the region of 2 mm above the DI water, versus the Ar gas flow rates ranged from 100 to 350 sccm, under the low electrical power of 4.9 W and driving frequency of 35 kHz. It is noted that these



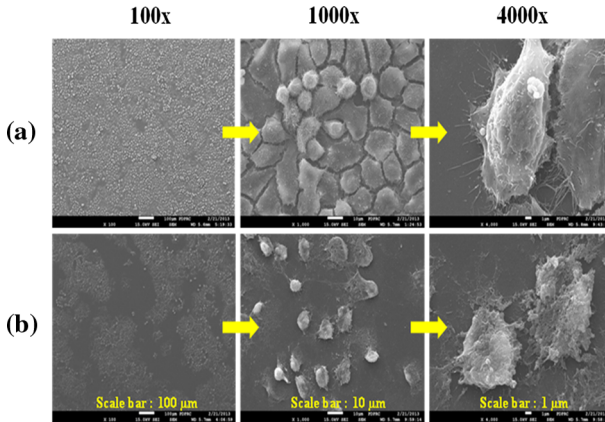
**Fig. 9** Density of OH radical species along with the OH absorption profiles in deionized (DI) water (a), Dulbecco's modified eagle medium (DMEM) (b), and  $1 \times$  phosphate buffered saline (PBS) (c) by ultraviolet absorption spectroscopy. As seen in the magnified view images of *dotted square* region, the ROS intensities from NO,  $O_2^{\bullet-}$  and  $H_2O_2$  are quite small in comparison with those for OH radical species inside the solutions

measurement values are within 5 % error ranges. For the gas flow rate of around 200–250 sccm, it is found that the density of hydroxyl OH radical species reaches the maximum value of  $2.6 \times 10^{15} \text{ cm}^{-3}$ . It is also noted that this density of OH radical species has been rapidly decreased to  $1.5 \times 10^{15} \text{ cm}^{-3}$  as the gas flow rate is increased to 350 sccm in this experiment. These OH densities are in relatively good agreement with other results of  $(0.3 \sim 7.5) \times 10^{15} \text{ cm}^{-3}$  reported by other groups under the low contents of water molecules <3 % in their employed gases of He,  $N_2$ , and  $N_2/O_2$  mixtures [4, 21, 22]. They have used a microwave frequency of 2.45 GHz [21, 22] and RF frequency of 13.56 MHz [18] with relatively high power greater than 100 W. However, we have used the low driving frequency of 35 kHz and low electrical power of 4.9 W in this experiment for the production of OH radical species inside the DI biosolutions by bombardment of the non-thermal atmospheric pressure plasma onto the DI water with Ar gas for various ranges of gas flow rates.

The density of the OH radical species inside the various biosolutions have been investigated when the Ar non-thermal plasma jet has been bombarded onto their surface. Figure 9 shows the emission and absorption profiles of the OH radical species inside the deionized (DI) water (a), Dulbecco's modified eagle medium (DMEM) (b), and  $1 \times$  phosphate buffered saline (PBS) (c) when the non-thermal plasma jet has been bombarded onto these biosolution surfaces. These emission and absorption optical signals have been measured at 2 mm below the biosolutions. It is noted here for the wavelength ranges between the 220 and 260 nm inside the biosolutions that there are emission profiles of



**Fig. 10** Temporal emission behaviors of 309 nm for OH radical species above and below deionized (DI) water. It is noted that the life times for OH species are 3.2 and 6.5 μs above the DI water and below it, respectively



**Fig. 11** Scanning electron microscope images of the control (a) and the plasma treated (b) lung cancer cells (H460) with different magnification. Ar non-thermal plasma is exposed to DMEM surface for 1 min, and cells are located 2 mm below the surface. The morphological changes should be induced by the hydroxyl OH radicals, since only hydroxyl OH radical density is measured high to be  $1.1 \times 10^{16} \text{ cm}^{-3}$  at 2 mm below the DMEM surface

224 nm for the nitric oxide NO [17, 18], 245 nm for the superoxide anion  $\text{O}_2^{\bullet-}$  [19], and 254 nm for the hydrogen peroxide  $\text{H}_2\text{O}_2$  [20] as seen in the magnified view images of dotted square region of Fig. 9. However, their intensities are quite small in comparison with those for OH radical species inside the biosolutions. It is also noted in this experiment that the densities of the OH radical species inside the DI water, DMEM, and PBS are measured to be about  $2.1 \times 10^{16}$ ,  $1.1 \times 10^{16}$ , and  $1.0 \times 10^{16} \text{ cm}^{-3}$ , respectively, at 2 mm downstream the surface during non-thermal plasma operation under Ar gas flow 200 sccm.

Also we have investigated the life times for OH radical species above the DI water surface and inside it, respectively. Figure 10 shows the temporal emission behaviors of 309 nm for OH radical species above the DI water and below it under Ar gas flow of 200 sccm, along with the electrical current signals. It is noted that the hydroxyl OH radical species above the DI has been generated simultaneously with respect to on-time of electrical current, while the OH radical species below the DI are increased slowly with respect to on-time of electrical current. It is noted that the life times for OH species are found to be 3.2  $\mu\text{s}$  above the DI water and 6.5  $\mu\text{s}$  below that, respectively, with respective rising time of  $\sim 100$  and  $\sim 200$  ns, in this experiment. Also, the falling time for OH radical species generated inside the DI water is measured to be about 6  $\mu\text{s}$ , which is two times longer than 2.5  $\mu\text{s}$  above the water. These longer life times and falling times of OH inside the solutions are main reasons for the higher OH density since the OH could be generated by two main pathways of  $\text{UV} + \text{H}_2\text{O}^* \rightarrow \text{OH}$  and  $\text{UV} + \text{H}_2\text{O}_2^* \rightarrow \text{OH}$  inside the water in comparison with air environment, which results in higher density of OH than air environment. The detail investigations for this will be published soon elsewhere.

We have prepared the lung cancer cell (H460), which is immersed and adhered on the inner bottom surface of petri dish with DMEM media, whose depth is 2 mm from the surface for the investigation of influence of hydroxyl OH density on this cell. Figure 11 shows the morphology for the control lung cancer cell (H460), magnified by 100 $\times$ , 1,000 $\times$ , and 4,000 $\times$  (a), and the morphology changes in the plasma treated lung cancer cell (H460), magnified by 100 $\times$ , 1,000 $\times$ , and 4,000 $\times$ , for 1 min exposure to DMEM surface, where it is noted that the hydroxyl OH density is measured to be  $1.1 \times 10^{16} \text{ cm}^{-3}$  at the adhered cell location of 2 mm downstream (b), respectively. It has been observed that smooth flat surfaces for control lung cancer cells, as in Fig. 11a, has been collapsed and crushed with shrunken surfaces as shown in Fig. 11b by the mutual interaction of hydroxyl OH species with lung cancer cells, where the hydroxyl OH radicals are produced inside the solution by the plasma treatment on the solution surface. With adjustment of experimental conditions, it is found that the threshold OH density for apoptosis of H460 cells inside the DMEM is about  $0.3 \times 10^{16} \text{ cm}^{-3}$  under 1 min plasma exposure, which may be followed by mitochondrial damages as reported previously [25].

## Conclusions

Non-thermal atmospheric pressure plasma jet has been developed for biomedical research fields with less electrical power operation of 4.9 W and driving frequency of 35 kHz. This paper contains the very informative data for describing the basic properties of non-thermal plasma jet such as the electron temperature on the biosolution surface as well as density of hydroxyl OH radical species inside the biosolutions during plasma bombardment onto the surface. A simple CR model has been employed in this experiment to determine the electron temperature of non-thermal plasma jet operating at atmospheric pressure by using the relative emission intensities of only four 2p Ar lines. It is noted that the electron temperatures have been measured at the region of 2 mm above the biosolution surface. It is found that electron temperature has been measured to be about 0.8–1 eV as the argon gas flow rate is increased from 200 to 300 sccm, and it is slowly decreased beyond 300 sccm and reached to 0.9 eV at 350 sccm.

Especially, when non-thermal plasma jet is operating on the biosolution surface, we have investigated that various reactive oxygen species (ROS) and reactive nitrogen species

(RNS) have been generated near the biosolution surface as well as inside them. The emission lines of 224–280 nm from the nitric oxide NO, the 245 nm from the superoxide anion  $O_2^{*-}$  and  $N_2$  second positive system (C3IIu–B3IIg) emission lines ranged from 320 to 380 nm are shown to be drastically decreased inside the biosolution of 2 mm downward its surface. However, it is found that the 309 nm emission from the hydroxyl OH radical species gets stronger in the biosolution than that above the solution.

It is found at the region of 2 mm above the solution surface that the density of hydroxyl OH radical species reaches the maximum value of  $2.6 \times 10^{15} \text{ cm}^{-3}$  for the gas flow rate of around 200–250 sccm in this experiment. Also the density of the OH radical species inside the various biosolutions have been investigated when the argon non-thermal plasma jet has been bombarded onto their surface. The densities of the OH radical species inside the DI water and DMEM are also measured to be about  $2.1 \times 10^{16}$  and  $1.1 \times 10^{16} \text{ cm}^{-3}$ , respectively, at 2 mm downstream the surface under Ar gas flow 200 sccm in this experiment. The OH density inside the PBS solution has been measured to be about  $1.0 \times 10^{16} \text{ cm}^{-3}$  at 2 mm downstream the surface during non-thermal plasma operation. It is found that the hydroxyl OH radical species above the DI water has been generated simultaneously with respect to on-time of electrical current, while the OH radical species below the DI are increased slowly with respect to on-time of electrical current. The life times for OH species are measured to be 3.2  $\mu\text{s}$  above the DI water and 6.5  $\mu\text{s}$  below that, respectively, with respective rising time of  $\sim 100$  and  $\sim 200$  ns. Also, the falling time for OH radical species generated inside the DI water is measured to be about 2.3 times longer than that above the water. These characteristics of longer OH life time inside the DI water might result in higher density for OH radical species in comparison with that above it.

It has been observed that smooth flat surfaces for control lung cancer cells has been collapsed and crushed with shrunken surfaces by the mutual interaction of hydroxyl OH radicals, where these OH radical species are produced inside the solution by the plasma treatment on the solution surface. It is found in this experiment that the threshold OH density for apoptosis of H460 cells inside the DMEM is about  $0.3 \times 10^{16} \text{ cm}^{-3}$  under 1 min plasma exposure.

Furthermore, it is necessary and essential to investigate the standard reference criterion of hydroxyl OH critical density for various kinds of cancer cells to induce their apoptosis when we will use the non-thermal atmospheric pressure plasma for healthcare applications throughout the future works.

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