

RESEARCH ARTICLE

Open Access

Tumour T_1 changes *in vivo* are highly predictive of response to chemotherapy and reflect the number of viable tumour cells – a preclinical MR study in mice

Claudia Weidensteiner^{1,2,3*}, Peter R Allegrini², Melanie Sticker-Jantschkeff¹, Vincent Romanet¹, Stephane Ferretti¹ and Paul MJ McSheehy¹

Abstract

Background: Effective chemotherapy rapidly reduces the spin–lattice relaxation of water protons (T_1) in solid tumours and this change (ΔT_1) often precedes and strongly correlates with the eventual change in tumour volume (TVol). To understand the biological nature of ΔT_1 , we have performed studies *in vivo* and *ex vivo* with the allosteric mTOR inhibitor, everolimus.

Methods: Mice bearing RIF-1 tumours were studied by magnetic resonance imaging (MRI) to determine TVol and T_1 , and MR spectroscopy (MRS) to determine levels of the proliferation marker choline and levels of lipid apoptosis markers, prior to and 5 days (endpoint) after daily treatment with vehicle or everolimus (10 mg/kg). At the endpoint, tumours were ablated and an entire section analysed for cellular and necrotic quantification and staining for the proliferation antigen Ki67 and cleaved-caspase-3 as a measure of apoptosis. The number of blood-vessels (BV) was evaluated by CD31 staining. Mice bearing B16/BL6 melanoma tumours were studied by MRI to determine T_1 under similar everolimus treatment. At the endpoint, cell bioluminescence of the tumours was measured *ex vivo*.

Results: Everolimus blocked RIF-1 tumour growth and significantly reduced tumour T_1 and total choline (Cho) levels, and increased polyunsaturated fatty-acids which are markers of apoptosis. Immunohistochemistry showed that everolimus reduced the %Ki67⁺ cells but did not affect caspase-3 apoptosis, necrosis, BV-number or cell density. The change in T_1 (ΔT_1) correlated strongly with the changes in TVol and Cho and %Ki67⁺. In B16/BL6 tumours, everolimus also decreased T_1 and this correlated with cell bioluminescence; another marker of cell viability. Receiver-operating-characteristic curves (ROC) for everolimus on RIF-1 tumours showed that ΔT_1 had very high levels of sensitivity and specificity ($ROC_{AUC} = 0.84$) and this was confirmed for the cytotoxic patupilone in the same tumour model ($ROC_{AUC} = 0.97$).

Conclusion: These studies suggest that ΔT_1 is not a measure of cell density but reflects the decreased number of remaining viable and proliferating tumour cells due to perhaps cell and tissue destruction releasing proteins and/or metals that cause T_1 relaxation. ΔT_1 is a highly sensitive and specific predictor of response. This MRI method provides the opportunity to stratify a patient population during tumour therapy in the clinic.

Keywords: Biomarkers, MRI, MRS, T_1 , Animal models, Everolimus, Tumour

* Correspondence: claudia.weidensteiner@uniklinik-freiburg.de

¹Oncology Research, Novartis Institutes for Biomedical Research, Basel, Switzerland

²Global Imaging Group, Novartis Institutes for Biomedical Research, Basel, Switzerland

Full list of author information is available at the end of the article

Background

Biomarkers are crucial to the development of new drugs and optimization of the existing options, by facilitating selection of the population to treat, confirming proof-of-concept and acting as early markers of tumour-response. The latter can be provided in the clinic by non-invasive functional imaging, for example positron emission tomography (PET) measurements of 2'-deoxy-2'-[18 F] fluoro-glucose (FDG) and 3'-deoxy-3'-[18 F]fluorothymidine (FLT), dynamic contrast-enhanced magnetic resonance imaging for vascular parameters and diffusion-weighted imaging for apoptosis [1,2]. However, they are not always easy to implement, and furthermore may be inappropriate for the mechanism-of-action (MoA) of a particular drug and cannot always detect true responses to the treatment [3-6]. We have recently described a rapid, robust MRI-method, which detects the response of solid tumours to drugs with different MoA in several different experimental models [7]. The method quantifies the spin-lattice relaxation of protons (T_1) in tumours both rapidly and accurately using an IR-TrueFISP method. Across several models, the fractional change in tumour T_1 (ΔT_1) correlated with the percentage of cells positive for the antigen Ki67 (a marker of cycling cells), but not with other markers such as apoptosis, necrosis or blood volume, all of which showed no consistent change with drug-treatment [7]. Recently, a preclinical study in a neuroblastoma mouse model treated with three different drugs showed a consistent decrease in T_1 [8], and a clinical study reported a small decrease in T_1 in patients with colorectal cancer metastasis undergoing bevacizumab therapy [9].

To investigate further what ΔT_1 reflects about the tumour biology, we have compared ΔT_1 with magnetic resonance spectroscopy (MRS) markers of proliferation and apoptosis *in vivo* [10], as well as histology and immunohistochemistry *ex vivo* following treatment with the allosteric mTOR inhibitor, everolimus (Afinitor) in two different murine tumour models, RIF-1 and B16/BL6. Everolimus was selected for these studies because although the drug has significant clinical activity in several different types of cancer, there is currently no confirmed molecular marker that can stratify the patient population [11]. Using the RIF-1 model, we demonstrate that ΔT_1 is a highly sensitive and specific predictor of response to everolimus and also the microtubule stabilizer patupilone. Collectively, these data further suggest that incorporation of T_1 measurements in clinical trials should be an important aid to drug development and optimization of existing drugs.

Methods

Tumour Models

All animal experiments were carried-out strictly according to the local Swiss animal welfare regulations. The protocol

was approved by the local veterinary authorities (Kantonales Veterinäramt Basel-Stadt, permit number 1974). C3H/He female mice (20–25 g) and C57/BL6 mice (20 g) were obtained from Charles River (France) and were acclimatized to local conditions for at least one week prior to experiments. Three experiments were performed in the RIF-1 fibrosarcoma model in C3H/He mice, one experiment was performed in the B16/BL6 melanoma model in C57/BL6 mice. All animal experiments were performed under isoflurane anesthesia, and every effort was made to minimize suffering.

Tumour volume (TVol) and animal body-weight (BW) measurements were made at least twice per week including just before treatment (baseline) and the endpoint. TVol was determined using calipers to measure three orthogonal dimensions and applying the formula: $l^*h*w*\pi/6$.

Murine RIF-1 fibrosarcoma

Freshly cultured RIF-1 tumour cells were injected subcutaneously (5×10^6 in 50 μ L phosphate-buffered saline) in the upper thigh of anesthetized C3H/He mice, as previously described [12]. After 2 weeks, tumours were of sufficient size (at least 200 mm^3) for the studies and were divided into two equal groups and treated daily with compound or vehicle. Experiment 1: treatment with everolimus (n = 7) compared to vehicle (n = 7), experiment 2: treatment with everolimus (n = 8) compared to vehicle (n = 8), experiment 3, previously published in [7]: three different doses of patupilone (each group n = 8) compared to vehicle (n = 8).

Murine B16/BL6 melanoma

Freshly cultured B16/BL6 tumour cells expressing the enzyme luciferase were injected intra-dermally (5×10^4 in 1 μ L) into the dorsal pinna of both ears of anesthetized C57/BL6 mice as previously described [12,13]. These black melanoma cells rapidly metastasize from the primary ear tumour to the regional lymph-nodes, in particular the neck. After 2 weeks, mice were divided into two equal groups (n = 10) and treated daily with everolimus (10 mg/kg p.o.) or vehicle for 6 days (experiment 4). MRI was performed on the metastasis in the cervical lymph nodes on day 5. In one mouse in the vehicle group there was no measurable lymph node metastasis.

Compounds/drugs and their application

All compounds utilized in this study were obtained from the Novartis chemical department. The compounds and their respective vehicles were prepared each day just prior to administration to animals and the administration volume individually adjusted based upon animal body weight. Everolimus (RAD001) was obtained as a microemulsion and was freshly diluted in a vehicle of 5% glucose and administered by oral gavage (p.o.) to mice

daily in a volume of 10 ml/kg at 10 mg/kg. Patupilone (epothilone B, EPO906) was dissolved in polyethylene glycol-300 (PEG-300) and then diluted with physiological saline (0.9% w/v NaCl) to obtain a mixture of 30% (v/v) PEG-300 and 70% (v/v) 0.9% saline. Treatment with vehicle (PEG-300/saline) or patupilone (3, 5 or 6 mg/kg) was once weekly using an i.v. bolus of 2–3 sec in the tail vein.

Experimental design

Mice were divided into different treatment groups so that each group had the same mean TVol, and magnetic resonance (MR) measurements were made before treatment (baseline) i.e. day 0 and at the endpoint. For everolimus, the endpoint was day 5, and for patupilone it was day 7. T_1 was measured in all four experiments. MRS was performed in experiment 1 only. Bioluminescence was measured *ex vivo* in experiment 4 (see below). At the end of everolimus-experiment 1, animals were sacrificed by CO₂ inhalation, the tumours ablated and prepared for histology and immunohistochemistry (IHC) as previously described [7].

Magnetic Resonance *in vivo*

Animals were anaesthetised using 1.5% isoflurane (Abbott, Cham, Switzerland) in a 1:1 mixture of O₂/N₂ and placed on an electrically warmed pad for cannulation of one lateral tail-vein as previously described [7]. MRI experiments were performed on a Bruker DBX 47/30 or Avance 2 spectrometer (Bruker Biospin, Ettlingen, Germany) at 4.7 T equipped with a self-shielded 12 cm bore gradient system.

Quantitative T_1 imaging

The spin–lattice relaxation of protons (T_1) was measured with an inversion recovery (IR) TrueFISP (true fast imaging with steady state precession sequence, [14]) imaging sequence as previously described [7]. The basic sequence was a series of 16 TrueFISP images acquired at a time interval, TI, following a global 180° inversion pulse (TI = 210 ms to 5960 ms in 324 ms increments). Each TrueFISP image (one slice containing the central part of the tumour) was acquired with a flip angle α of 30°, a matrix size of 128 × 96, a field-of-view of 30 × 22.5 mm², a slice thickness of 2 mm, an echo time (TE) of 1.7 ms, and a repetition time (TR) of 3.4 ms. Pixelwise T_1 calculation was done using the method described in [15]. A region of interest (ROI) comprising the entire tumor was drawn manually on the resulting T_1 map and the mean T_1 of the central tumour slice was calculated in this ROI. MR image analysis was performed off-line with in-house written software based on IDL 6.0 programming environment (Research Systems Inc., Boulder, CO, USA).

¹H-MR spectroscopy

Localized shimming with FASTMAP method was performed on a 2.5 mm³ voxel to obtain line widths of <20 Hz. Point resolved spectroscopy (PRESS) experiments at the same voxel position (voxel size = 8 mm³, TE = 20 msec, TR = 1500 msec, SW = 4000 Hz, TD = 2048, with external volume suppression) were performed. One spectrum was acquired with water suppression (400 averages) and one spectrum without water suppression (1 average). The total time for MRS was 10–12 min for each mouse. The water signal (one peak) of the non-suppressed spectrum was used as an internal reference for relative quantification of metabolites using the metabolite to H₂O ratio (Cho/H₂O for choline, etc.). Peaks in the water-suppressed spectrum were identified by their chemical shifts, so total choline (Cho) was at 3.2 ppm, CH₃-lipids at 0.9 ppm, CH₂-lipids at 1.3 ppm, creatine at 3.0 ppm, and polyunsaturated fatty-acids (PUFA) at 5.3 ppm and very weakly at 2.8 ppm; however the latter peak was not used for any calculations.

Histology and immunohistochemistry

A tumour slice of 3–4 mm thickness was cut from the largest circumference of the tumour, immersion-fixed in 4% (w/v) phosphate-buffered formalin (pH 7.4; J.T. Baker, Medite, Service AG, Dietikon, Switzerland) at 4°C for 24 hours and processed into paraffin as previously described [4]. IHC was performed on paraffin sections of 3 μm using the following antibodies for detection of (i) cleaved Caspase-3 (rabbit polyclonal antibody #9661, Cell Signaling, Danvers, MA, USA) (ii) Ki67 (rat monoclonal antibody, clone TEC3, #M7249, DAKO, Glostrup, Denmark) and (iii) CD31 (rabbit polyclonal antibody, #E11114, Spring Biosciences, Pleasanton, CA, USA).

Image acquisition and analysis of histological slices

For quantification, the entire section was scanned using the MiraxScan system (Carl Zeiss AG, Jena, Germany). The absolute size of viable, necrotic and complete tissue areas was measured on the full scans using MiraxViewer software (Carl Zeiss AG, Jena, Germany). Quantification of Ki67 positive and negative nuclei in the complete viable areas was performed in a fully automated manner with TissueMap software at Definiens AG, Munich, Germany. Results were summarized as the total area, percentage-viable and percentage-necrotic area, total number of nuclei and the cell density (number of nuclei per mm²) in both the viable and total (including therefore necrotic) areas. Cleaved caspase-3 positive particles were quantified as positive pixels per total pixels in a semi-automated fashion with the AnalySIS[®] FIVE software (OlympusSIS, Münster, Germany) on six images (346.7 × 260 μm² each) per section excluding necrotic areas and border zones of necrotic areas. CD31 stained

slides were scanned with the Aperio ScanScopeXT slide scanner (Aperio, Vista, CA, USA) and vessels were quantified with the Aperio ImageScope software, using the Microvessel Analysis v1 Algorithm.

Bioluminescence

Because of the black pigmentation of the C57/BL6 mice, bioluminescence (BioL) could not adequately be measured *in vivo* and therefore was determined *ex vivo* as follows. After 6 days, the cervical lymph-nodes were removed and weighed and then iced. Individual lymph-nodes were homogenized at 4°C with 1 mL cold phosphate-buffered saline (without Ca²⁺ and Mg²⁺), rinsed in the same buffer, and 200 µl triplicates placed in a 96-well plate with 50 µl D-luciferin (1 mg/mL). BioL was measured at an emission wavelength of 560 nm using the imaging chamber of the IVIS™ system (Caliper Life Sciences Inc, Hopkinton, MA, USA) for 1 min at room temperature.

Data analysis

Results are presented as mean ± SEM except where stated and all available data are shown. The T/C ratio is commonly used to quantify tumour growth inhibition, where T and C represent the means of the relative tumour volumes (tumour volume divided by its initial volume) of the treatment and control mice, respectively [16]. Longitudinal changes, such as in tumour volume (Δ TVol) or in T₁ (Δ T₁), were expressed as change between endpoint and baseline divided by value at baseline (fractional change in %). The T/C ratio was calculated for all parameters. For parameters measured at one time point only (such as histological read-outs), T/C was calculated as ratio of means of treatment and control mice, respectively. Differences between groups were analysed using a 2-tailed t-test. For the *in vivo* biomarker analyses which involved longitudinal analyses in the same animals, differences were analysed by a) 2-way repeated measures ANOVA and b) t-test at the endpoint; the latter method is therefore associated with the respective T/C. The different dose groups in experiment 3 were tested with 1-way ANOVA vs. control group. Quantification of the linear-relationship between the various parameters measured *in vivo* and *ex vivo* were analysed by Pearson's correlation to provide the correlation coefficient (r) and the significance (p). Application of the non-parametric Spearman's correlation did not affect the results except in one case (see Results). To facilitate comparison of PUFA levels which were not always detectable, a 2-sided Fisher's exact test was also used. For all tests, the level of significance was set at p < 0.05 (two-tailed) where *p < 0.05, **p < 0.01, ***p < 0.001 versus vehicle.

To determine the sensitivity and specificity of a change in the imaging marker T₁ as a marker of tumour response to treatment, receiver-operator curves (ROC) were generated

[17,18] using Graphpad Prism (GraphPad Software, La Jolla, CA, USA) considering mice treated with the drugs everolimus (experiment 1 and 2) or patupilone (experiment 3). Briefly, responders (R) to drug-treatment were defined as showing no change or regression, in TVol, defined as Δ TVol ≤ 10%, while all others were considered non-responders (NR). Each of these tumours was then classified as R or NR by the Δ T₁ at different discrete cut-offs to generate at each Δ T₁ value a table of positive and negative predictions for determination of specificity and sensitivity at each value. The plot of 1-specificity versus sensitivity generated the ROC curve and the area under this curve (AUC) was quantified by the trapezoidal method.

Results

Effects of everolimus on MRI and MRS biomarkers in RIF-1 tumours *in vivo*

Murine RIF-1 tumours grew rapidly having a 2.5-fold increase in tumour volume after just 5 days, but daily treatment with everolimus (10 mg/kg p.o.) strongly inhibited tumour growth causing essentially stable disease at the 5 day endpoint with a T/C of 0.05 (Table 1). Both groups had a significant difference in TVol at baseline (slightly larger TVol in the treatment group), but this did not have an effect on the results, as can be seen in Table 1. Quantification of tumour T₁ by MRI at baseline gave a mean ± SD of 2301 ± 100 msec (both groups, n = 14) which showed no significant change in vehicle-treated mice, but was reduced in 7/7 mice treated with everolimus providing a small but highly significant mean decrease of 10 ± 2% after 5 days treatment (Figure 1, Table 1).

¹H-MRS on the same tumours at the same time-points was also performed to provide signals for total choline, creatine, as well as polyunsaturated lipids (PUFA) and saturated (CH₂ and CH₃) lipids (Figure 2A). The strong water signal (unsuppressed) was used to provide quantitative information as ratios (see Methods). This data showed that creatine and saturated lipids did not change in either treated-group (Table 1). However, total choline (Cho) in most cases (5/7) decreased in everolimus-treated tumours, with a mean change in choline Δ Cho/H₂O of 27 ± 15% (statistically significant only in ANOVA, not in t-test; Figure 2B,C). The PUFA peaks were broad and of low intensity (Figure 2A) and were only detectable at baseline in 1/7 tumours for each group. However, after 5 days treatment they were more prevalent, permitting quantification in 2/7 vehicle-treated and 5/7 everolimus-treated tumours which showed a T/C of 2.2 (Table 1). This data was obviously rather variable and scarce due to the limit-of-detection by MRS and there was no significant difference between the two groups although a two-way repeated-measures ANOVA (as used for T₁ and Cho)

Table 1 Summary of RIF-1 measurements *in vivo* and *ex vivo*

Parameter	Vehicle		Everolimus		T/C
	Day 0	Day 5	Day 0	Day 5	
TVol (mm ³)	447 ± 75	1118 ± 150	706 ± 85	736 ± 100	0.05***
T ₁ (msec)	2266 ± 46	2265 ± 30	2335 ± 23	2090 ± 45	0.89**
choline/H ₂ O [a.u.]	2.72 ± 0.18	2.72 ± 0.2	2.6 ± 0.12	1.82 ± 0.32	0.73
CH ₂ /H ₂ O [a.u.]	6.44 ± 0.85	7.3 ± 1.17	6.89 ± 0.35	11.0 ± 1.5	1.3
CH ₃ /H ₂ O [a.u.]	2.56 ± 0.43	2.86 ± 1.74	3.06 ± 0.34	4.87 ± 0.72	1.2
PUFA/H ₂ O [a.u.]	0.1 ± 0.1	0.37 ± 0.24	0.25 ± 0.25	0.8 ± 0.39	2.2
creatine/H ₂ O [a.u.]	1.27 ± 0.15	1.14 ± 0.05	1.07 ± 0.06	0.89 ± 0.09	0.9
total area (mm ²)	-	65.8 ± 10.0	-	43.6 ± 5.6	0.66
viable area (mm ²)	-	52.1 ± 9.4	-	33.1 ± 4.7	0.64
%necrosis	-	21.5 ± 6.1	-	24.9 ± 3.3	1.16
total cells (thousand)	-	489 ± 82	-	328 ± 48	0.67
cells/viable mm ²	-	9671 ± 454	-	9923 ± 562	1.03
%Csp ⁺ area	-	0.39 ± 0.07	-	0.27 ± 0.02	0.7
BV per mm ²	-	728 ± 159	-	768 ± 37	1.06
%Ki67 ⁺ cells	-	44.6 ± 2.5	-	26.5 ± 1.0	0.59***
Ki67 ⁺ cells/mm ²	-	4274 ± 205	-	2614 ± 141	0.61***
Ki67 ⁻ cells/mm ²	-	5396 ± 457	-	7309 ± 462	1.35*

C3H mice bearing RIF-1 tumours were treated with everolimus (10 mg/kg/day, n = 7) or vehicle (n = 7) for 5 days prior to sacrifice. Tumour volume, T₁ and the various MRS parameters were quantified prior to treatment (day 0) and after 5 days treatment. Animals were then culled and the tumours ablated and prepared for immunohistochemistry as described in Methods. After immunostaining for Ki67 and cleaved caspase-3, the entire tumour sections were scanned to provide viable and necrotic areas in mm². The number of cells and the number and percentage staining for Ki67 and caspase-3 is shown only for the viable area but essentially identical results were obtained if the entire area was used. Blood vessels (BV) were quantified from CD31 stained slices. All results show the mean ± SEM for each tumour, significant changes are indicated by emboldened numbers where *p < 0.05, **p < 0.01, ***p < 0.001 comparing the two treatment group means (2-tailed t-test).

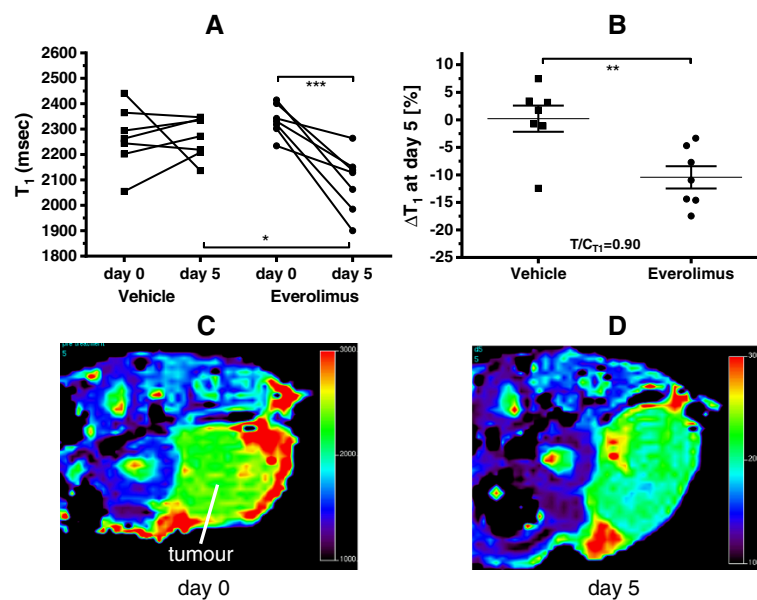


Figure 1 Everolimus decreases the T₁ of RIF-1 tumours. C3H mice bearing RIF-1 tumours were treated with everolimus (10 mg/kg/day) or vehicle for 5 days and the spin-lattice relaxation of protons (T₁) in tumours was measured on day 0 and at the endpoint day 5. Results show the individual values for each tumour, n = 7 per treatment group (A) and the mean ± SEM fractional change ΔT₁ for each treatment (B), where *p < 0.05, **p < 0.01, ***p < 0.001 as shown. Panel C & D show an MRI-derived T₁ map from a representative RIF-1 tumour (arrow) before (C) and after (D) treatment with everolimus.

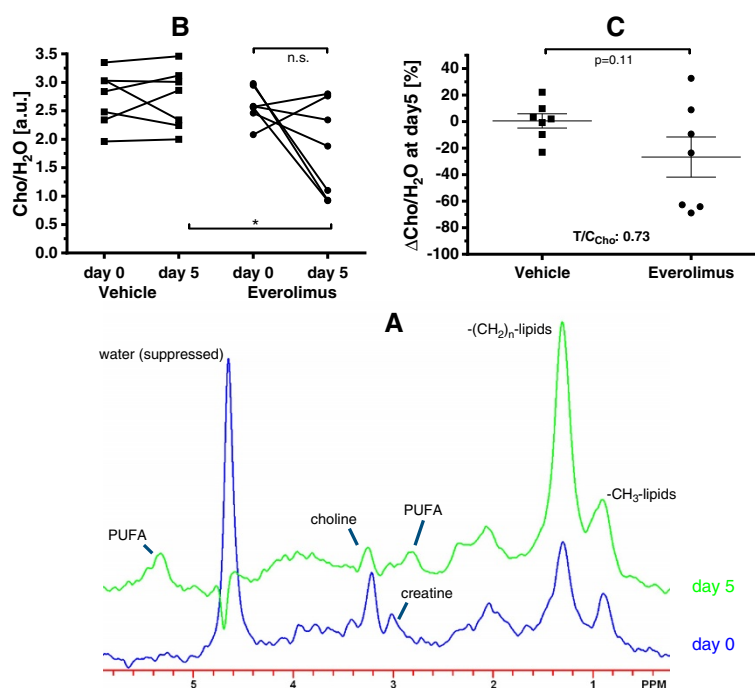


Figure 2 Everolimus decreases the Cho/H₂O ratio of RIF-1 tumours. C3H mice bearing RIF-1 tumours were treated with everolimus (10 mg/kg/day) or vehicle for 5 days and the ratio of total choline to (unsuppressed) water (Cho/H₂O) in tumours was measured on day 0 and at the endpoint day 5. Panel A shows a ¹H-MRS spectrum from a representative RIF-1 tumour before and after treatment with everolimus. Graphs show the individual values for each tumour, n = 7 per treatment group (B) and the mean ± SEM fractional change ΔCho/H₂O for each treatment (C), where *p < 0.05 as shown.

showed that everolimus significantly increased PUFA (p = 0.007), a parameter that has also been associated with apoptosis [10].

Ex vivo analyses of everolimus on RIF-1 tumours

At the endpoint, the ablated tumours were prepared for histology. Since everolimus inhibited tumour growth, there was of course a reduction in the total and viable area and consequently a reduction in the total cell number examined by IHC comparing everolimus-treated to vehicle-treated mice (Table 1, Figure 3), although these did not quite reach significance (p = 0.1). The cell density (cells per mm²) in the viable (or total) area and the %-necrosis was the same in each group (Table 1). The number of cells positive for the proliferation marker Ki67 was relatively high in vehicle-treated mice (45 ± 3%) and everolimus caused a clear and highly significant decrease in the total number and %Ki67⁺ cells to 27 ± 1% (Table 1; Figure 3, first and second row). Correspondingly, there was a significant increase in the number of Ki67⁻ cells. In contrast, there was a very low level of apoptosis as measured by caspase-3 staining in these tumours (<1%) and this was not affected by everolimus treatment (Table 1; Figure 3, third row). The number of blood-vessels (BV) per slice was rather variable, particularly in the vehicle-group, and a comparison of the blood-vessel density

between treatment groups showed no effect from everolimus (Table 1; Figure 3, last row CD31).

Relationships between RIF-1 biomarkers and tumour response

As previously observed for several different experimental models and drugs, including everolimus [7], the change in T₁ (ΔT₁) was highly significantly (p = 0.0032) positively correlated with the change in RIF-1 tumour volume (ΔTVol), see Figure 4A, but there was no significant correlation between ΔCho/H₂O and ΔTVol. Correlation of ΔT₁ and ΔCho/H₂O reached significance (r = 0.58, p = 0.028), see Figure 4B, although not when a Spearman correlation was applied (r = 0.43, p = 0.13). ΔT₁ showed a significant positive correlation with the %Ki67⁺ cells (Figure 4C), a similar level of correlation existed between %Ki67⁺ and ΔCho/H₂O (r = 0.56, p = 0.036); and of course negative correlation with the %Ki67⁻ cells (graphs not shown). There was no significant relationship between basal T₁ value and ΔTVol in keeping with previous observations in many different preclinical models [7] that basal T₁ cannot predict response. The final T₁ or ΔT₁ was unrelated to cell density, or indeed the total number of cells, with flat lines of correlation and wide scatter (results not shown). Thus, ΔT₁ was unrelated at the endpoint to cell density or the extracellular space but was related to the remaining

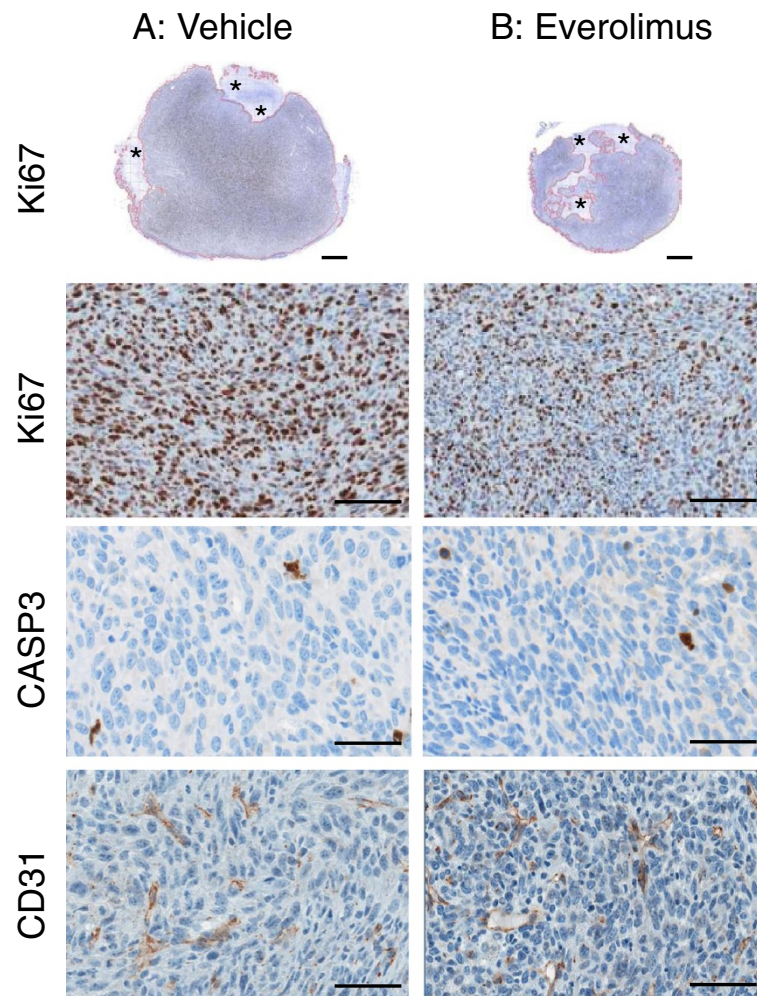


Figure 3 Immunohistochemistry in RIF-1 tumours after everolimus or vehicle treatment. C3H mice bearing RIF-1 tumours were treated with vehicle (A, left column) or everolimus at 10 mg/kg/day (B, right column) for 5 days prior to sacrifice (n = 7 per group). Tumours were ablated and prepared for immunohistochemistry as described in Methods. The entire sections were scanned. Ki67-stained slices of one representative tumour from each treatment (scalebar = 1 mm) are shown in row 1. Viable tumor tissue is outlined in red and necrosis regions are marked with asterisks. Percentage of Ki67-positive cells was 46% and 26% and the total tumour area was 43.9 mm² (8% necrosis) and 22.4 mm² (19% necrosis) for the vehicle-treated and everolimus-treated mice, respectively. Magnified sections stained for Ki67 (scalebar = 50 μm), cleaved caspase-3 (CASP3, scalebar = 25 μm), and CD31 (scalebar = 25 μm) are shown below in row 2, 3, and 4, respectively. There was no difference between the groups in apoptosis (CASP-3 staining) and blood-vessel density (CD31 staining).

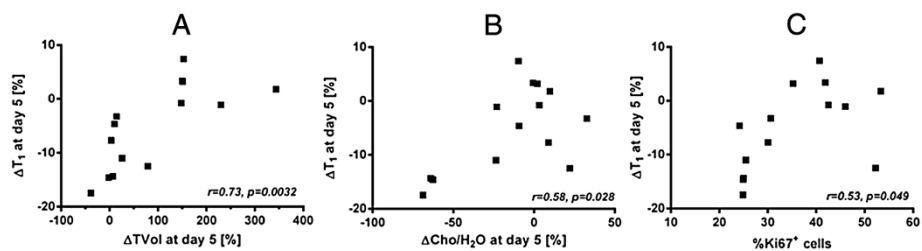


Figure 4 Inter-relationships of biomarkers following everolimus or vehicle treatment of RIF-1 tumours. Graphs A-C show Pearson correlations with the associated r and p values between the fractional change in T₁ (ΔT_1) and the fractional change in tumour volume ($\Delta TVol$), the fractional change in total choline ($\Delta Cho/H_2O$), and percentage of Ki67 positive cells, respectively, after 5 days of everolimus or vehicle treatment (n = 7 per group) of C3H mice bearing RIF-1 tumours.

number of proliferating cells (and negatively correlated to the number of non-proliferating cells). PUFA levels, which also tended to change with treatment could not be formally correlated since the data was categorical, but a Fisher's exact test showed a significant association between Cho and PUFA ($p = 0.02$) i.e. proliferation decreased as apoptosis increased.

Sensitivity and specificity of ΔT_1 as a response biomarker in RIF-1 tumours

Correlations and linear regression provide indications of whether a biomarker could be used to predict response, but a receiver operating characteristic curve (ROC) can be more definitive in terms of the specificity and sensitivity of the marker. To generate such a curve for everolimus, data from experiments 1 and 2 was pooled from RIF-1 tumours (Figure 5A). The left panel shows the $\Delta TVol$ for mice treated with vehicle or everolimus and the right panel the ΔT_1 in those tumours from day 0 to day 5 ($n = 15$ vehicle, $n = 13$ everolimus; in the everolimus group of experiment 2 one mouse died before endpoint and T_1 measurement failed in another mouse). Responders to everolimus treatment were defined as showing a maximum change in $\Delta TVol$ of +10% (stable disease or regression), so giving 5R and 8NR and providing the 'gold-standard'. Each of these 13 tumours was then classified as a R or NR by the ΔT_1 using different discrete cut-offs ranging from -16.5% to -2.5% to generate at each ΔT_1 value a table of positive and negative predictions for determination of specificity and sensitivity at each value, see for example Table 2A. The plot of 1-specificity versus sensitivity generated the ROC curve and the area under this curve (AUC) was quantified giving a value of 0.84 which is considered to be very good predictive ability [17].

The same approach was used to analyse data already published [7] from the cytotoxic patupilone on the same RIF-1 tumour model. In this case, a dose-response was used (Figure 5B, left panel) and R and NR identified in the same way giving 7R and 13NR (from the 20 tumours). The right panel (Figure 5B) shows the ΔT_1 in those tumours from day 0 to day 7 ($n = 6-8$ per dose). Using once more discrete ΔT_1 values from -24% to 8.5% a table of positive and negative predictions was generated (see for example Table 2B) and the ROC plotted (Figure 5B). The AUC of this plot was 0.97 confirming outstanding predictive ability for ΔT_1 in the RIF-1 model.

Relationship between bioluminescence and T_1 in B16/BL6 tumours

Everolimus inhibited growth of B16/BL6 lymph-node metastases after 6 days daily treatment leading to a T/C ratio for the weight of the dissected metastases of $T/C_{weight} = 0.60$ and this was associated with a highly

significant decrease in the T_1 of the metastases of $19 \pm 3\%$ (Figure 6A,B). T_1 measurement failed in one mouse treated with vehicle and in two mice treated with everolimus resulting in $n = 8$ ΔT_1 values in each group. Bioluminescence from these lymph-nodes measured *ex vivo* was also significantly decreased (Figure 6C) and this correlated significantly with the ΔT_1 (Figure 6D). Since the enzyme luciferase is only located within the melanoma cells, the bioluminescence should only reflect the viable tumour cells which supports the notion that a change in T_1 is an indirect measurement of the viable and/or proliferating cell fraction.

Discussion

We have previously shown that a small but highly significant decrease in the mean spin-lattice relaxation of protons (T_1) of experimental tumours induced by various different types of chemotherapy is strongly correlated with the change in tumour volume and also the immunohistochemical proliferation marker Ki67 [7]. Furthermore, in the RIF-1 model the antimetabolite 5FU also decreased levels of the proliferation marker choline and this too was correlated with the change in T_1 (ΔT_1). The data presented here on RIF-1 and B16/BL6 tumours confirm these observations for the allosteric mTOR inhibitor everolimus, providing further evidence that ΔT_1 reflects the number of remaining proliferating tumour cells following successful chemotherapy. The greater the decrease in T_1 , the lower the percentage of proliferating cells after therapy. In the previous report, a sample area (10%) of an *ex vivo* tumour slice was examined histologically, and thus, true cell density and also therefore the overall extracellular space could not be assessed either. In two models, using the cytotoxic patupilone on murine RIF-1 and rat mammary BN472, there were trends for cell-density to decrease by approx. 10% but neither reached significance [7]. In this report, we have made a detailed histological study of the effect of everolimus on RIF-1 tumours grown s.c. in murine C3H mice.

RIF-1 cells are sensitive to everolimus with an IC_{50} *in vitro* of 2.6 ± 1.6 nM (insensitive cells have an $IC_{50} > 1$ μM , see references [19,20]), but this is still not as sensitive as the endothelial cells which have $IC_{50} < 1$ nM, which likely explains the fact that everolimus has anti-tumour cell as well as anti-angiogenic properties [19]. Daily treatment of mice bearing RIF-1 tumours caused tumour stasis, and consistent with this, histology at the endpoint of 5 days showed a decrease in total tumour area and a proportional decrease in the viable area of approx. 35% compared to vehicle (both not significant, $p < 0.1$). However, the total number of cells showed a similar trend for a decrease in proportion ($p < 0.1$) and thus the overall cell density in the viable areas was unchanged. Since necrosis was also not affected by everolimus

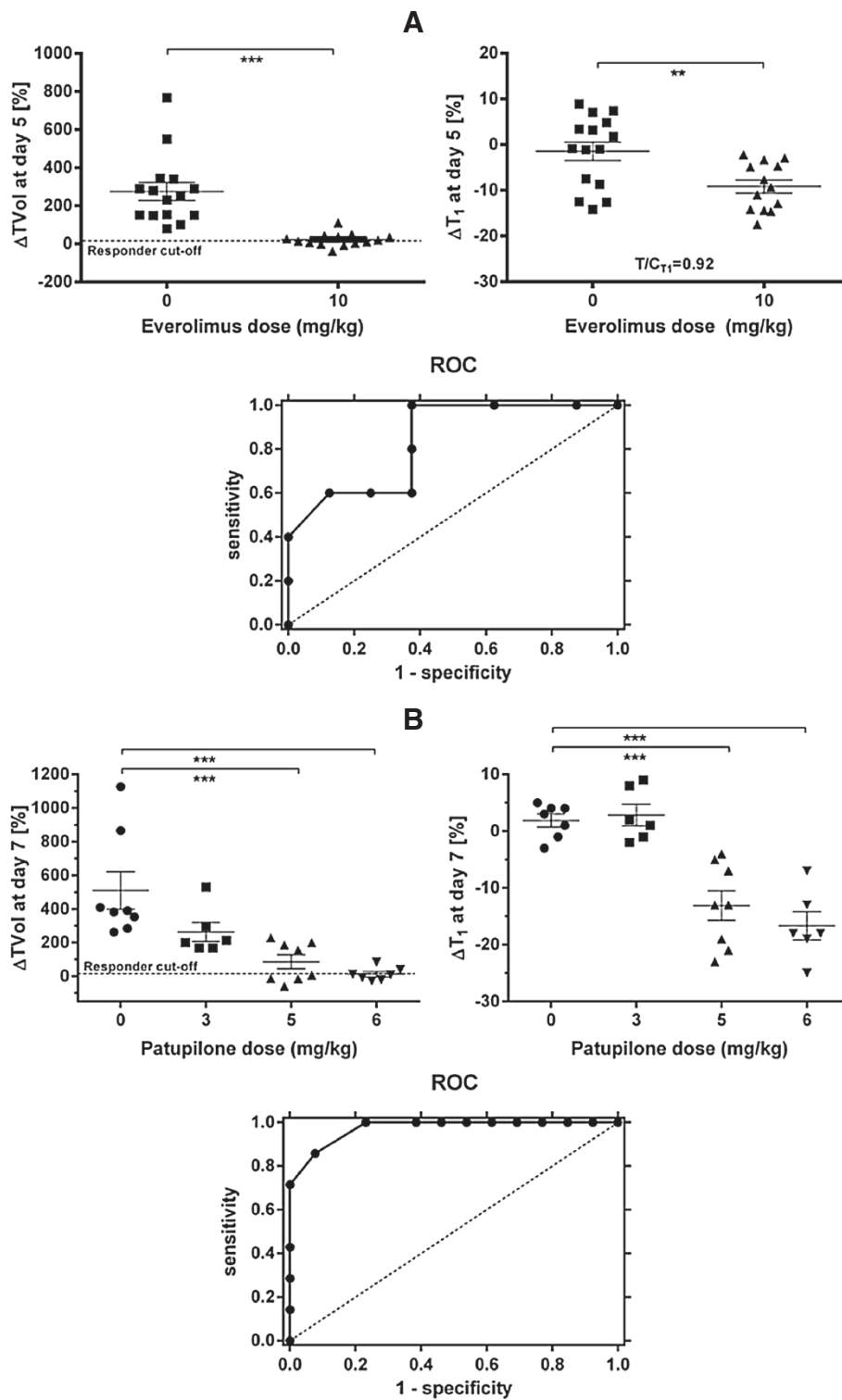


Figure 5 (See legend on next page.)

(See figure on previous page.)

Figure 5 Sensitivity and specificity of ΔT_1 for everolimus and patupilone chemotherapy in the RIF-1 tumour model. **A.** C3H mice bearing RIF-1 tumours were treated with everolimus (10 mg/kg/day) or vehicle for 5 days and TVol and the spin-lattice relaxation of protons (T_1) in tumours was measured on day 0 and at the endpoint day 5 (n = 15 per group on day 0). In the everolimus group, one mouse died before endpoint and T_1 measurement failed in another mouse on day 5. Results show the change in TVol ($\Delta TVol$) (left panel) and the fractional change in T_1 (ΔT_1) (right panel) for each treatment on day 5, where **p < 0.01, ***p < 0.001 as shown. The ROC plots 1-specificity versus sensitivity for tumours treated with everolimus only and has an AUC = 0.84; the dashed line is the line of equivalence where the AUC = 0.5. **B.** C3H mice bearing RIF-1 tumours were treated with patupilone (3, 5 or 6 mg/kg i.v. bolus once) or vehicle and TVol and T_1 in tumours was measured on day 0 and at the endpoint day 7 (n = 8 per group). In some mice, T_1 could not always be determined and thus there were only n = 6 or 7 per group for analysis. Results show the $\Delta TVol$ (left panel) and the ΔT_1 (right panel) for each treatment on day 7 where ***p < 0.001 as shown. The ROC plots 1-specificity versus sensitivity for tumours treated with different doses of patupilone and has an AUC = 0.97; the dashed line is the line of equivalence where the AUC = 0.5.

(non-significant increase of 20%), this analysis showed that cell density and the extracellular space were unaffected. Many previous experiments *in vitro* and using human tumour xenografts *in vivo* have shown that T_1 is sensitive to a) the amount of water in the extracellular space (but not intracellular) and b) the amount of protein in the water [21-25]. It is well recognised that inhibition of mTOR (the molecular target of everolimus) causes a decrease in cell size [26], because cell cycle progression is blocked at G1 thus inhibiting protein synthesis and cell growth. Consequently, cell density might not change, but the extracellular space could increase. Unfortunately we could not measure the average cell size because defining where one cell ends and another begins is difficult and there was no automatic programme for such an approach. But in any case, an increase in extracellular space would lead to an increase rather than a decrease in T_1 [21-25], suggesting that if cell size changes occurred they could not explain the T_1 decrease that we have always observed following successful chemotherapy with many different agents [7]. This suggests to us, that tumour cell and vascular destruction leads to the release of proteins and also paramagnetic ions into the extracellular space which causes the decrease in T_1 ; an effect which has been shown *in vitro* [22]. However, everolimus did not cause a decrease in the blood vessel density, as has been seen in several other tumour models [20,27-29], although this does not rule out an effect on the functional vasculature (previously measured as low in RIF-1 tumours [30]) and/or that early vascular changes had normalised by day 5. Also in this model, there was no clear evidence of increased tumour cell kill since caspase-3 levels were unaffected, although there did appear to be a strong trend for an increase in the PUFAs of everolimus-treated tumours which has been associated with apoptosis in other experimental models [10].

Immunohistochemistry (IHC) showed that approx. half of vehicle-treated RIF-1 tumour cells were positive for the nuclear antigen Ki67. Ki67 is considered to be a proliferation marker since it is expressed in all cycling cells (G1, S and G2M) but not therefore in cells in G0, and is a convenient IHC tool in the clinic for assessing tumour growth and response [31,32]. Given that the

effect of mTOR inhibition is to block G1, it was not surprising that everolimus caused a marked decrease in the %Ki67⁺ cells whether expressed as total number or density and there was a proportional increase in the cells negative for Ki67. Everolimus also decreased levels of total choline (Cho) in RIF-1 tumours, which is another marker of viable and proliferating cells, in this case reflecting membrane turnover. Cho tends to be higher in tumour than normal tissue [33] and successful chemotherapy has also been shown to decrease in Cho in both experimental models [7,8,10] and the clinic [34,35]. In the RIF-1 tumours, these proliferation markers correlated significantly with each other as well as with the ΔT_1 , supporting the notion that ΔT_1 is a surrogate of the remaining number of proliferating cells in a tumour after therapy even though our histological analysis suggests that it cannot be measuring cell number or density directly. Support for this hypothesis came from the B16/BL6 model treated with everolimus where again the

Table 2 T_1 sensitivity and specificity tables for changes in RIF-1 tumour volume following everolimus or patupilone treatment

A. Everolimus: using a ΔT_1 of -8%			
ΔT_1	$\Delta TVol$		Total
	Positive	Negative	
Positive	5	3	8
Negative	0	5	5
Total	5	8	13

B. Patupilone: using a ΔT_1 of -8%			
ΔT_1	$\Delta TVol$		Total
	Positive	Negative	
Positive	7	3	10
Negative	0	10	10
Total	7	13	20

A. Everolimus: The prevalence (total positive/all) = 0.38. The sensitivity = 1.0 and the 1-specificity = 0.38, giving a positive prediction value of 0.63 and a negative prediction value of 1.0 at this ΔT_1 cut-off of -8%.
B. Patupilone: The prevalence (total positive/all) = 0.35. The sensitivity = 1.0 and the 1-specificity = 0.23, giving a positive prediction value of 0.70 and a negative prediction value of 1.0 at this ΔT_1 cut-off of -8%.

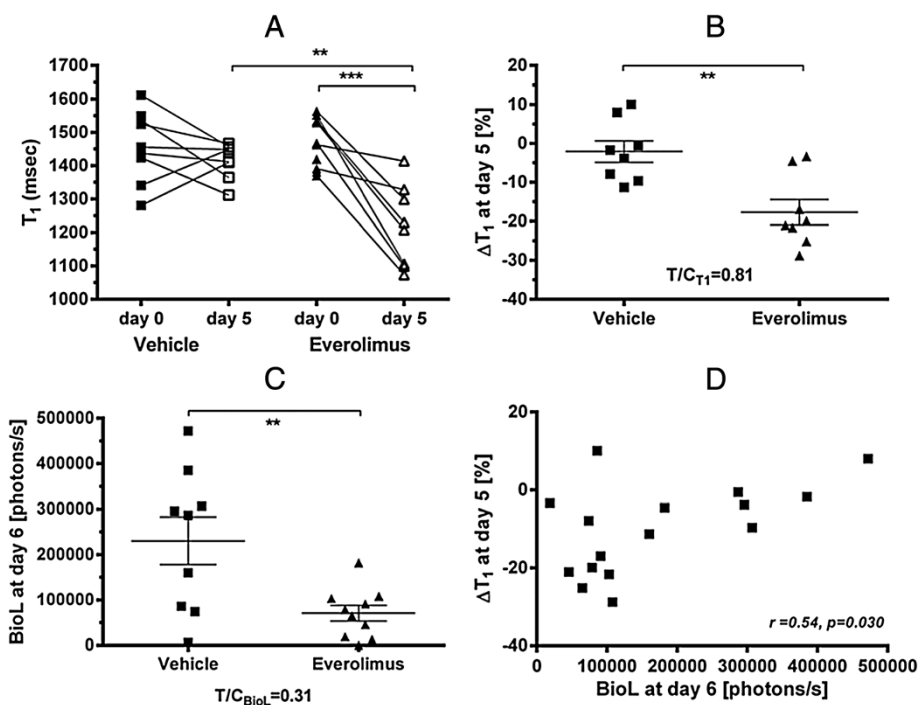


Figure 6 Everolimus decreases the T_1 and bioluminescence of cervical B16/BL6 melanoma metastases. C57/BL6 mice bearing B16/BL6 melanomas were treated with everolimus (10 mg/kg/day) or vehicle for 6 days and the spin-lattice relaxation of protons (T_1) in tumours was measured on day 0 and at the endpoint day 6. Lymph-nodes were removed and extracted for measurement of bioluminescence (BioL) as described in Methods. Results show the mean \pm SEM, and the individual T_1 values (A) and bioluminescence (C), the fractional change in T_1 (ΔT_1) for the treatments (B), and the Pearson correlations (with the associated r and p values) between BioL and ΔT_1 (D), where $**p < 0.01$, $***p < 0.001$ as shown.

decrease in bioluminescence, which measures viable tumour cell number, was correlated to the ΔT_1 .

It is worth repeating that we have found that six different types of chemotherapy including anti-metabolites, inhibitors of mTOR, microtubules, VEGF-R, PI3K and HSP90 [7] [and unpublished] in several different tumour-types implanted in both mouse and rat hosts, all showed a decrease in T_1 in response to successful chemotherapy i.e. characterized by a significant change in TVol in comparison to vehicle-treated tumours. Furthermore, where a tumour was resistant to that particular type of chemotherapy (paclitaxel and patupilone), there was no change in T_1 [7]. This suggests that ΔT_1 is a generic marker of tumour response, because, as discussed above, it reflects overall tumour destruction. But, what is the level of sensitivity and specificity i.e. how useful could such a method be in the clinic? To answer this question, we used receiver-operating-characteristic curves (ROC) to analyse two different models in which mice bearing RIF-1 tumours were treated with either a single dose of everolimus or three different doses of patupilone. In both cases, the ROCs had a large area-under-the-curve (AUC) of 0.84 and 0.97 which is considered of very good to outstanding predictive ability [17]. Consider for comparison, IHC markers of the mTOR pathway to predict everolimus activity *in vitro* using cell lines in which ROC-AUCs of 0.86-0.88 were determined

[20]; also excellent predictive activity but no better or even lower than that we have shown here. Indeed, with our data, if a cut-off of an 8% decrease were selected (i.e. $\Delta T_1 = -8\%$), then the sensitivity to both drugs would be perfect in this model at 1.0 i.e. providing a negative predictive value of 100%. In other words, after two MRI-scans one could completely eliminate from the study any tumours with a T_1 decrease smaller than 8% since these should not benefit from further treatment.

Conclusion

T_1 showed a decrease in response to successful chemotherapy in several tumour models using various drugs. Analysis of histological and bioluminescence data from tumours treated with everolimus indicate that ΔT_1 is a generic marker of tumour response reflecting overall tumour destruction and the decreased number of proliferating cells.

The excellent negative predictive value of ΔT_1 suggests that the method should be tested in the clinic, for example wherever MRI is being used anyway to determine tumour size. Potentially, it provides the opportunity to stratify a patient population after the first cycle of treatment to increase the effective response-rate as well as to save resources by avoiding treatment of patients who are unlikely to respond.

Abbreviations

AUC: Area under curve; BioL: Bioluminescence; BV: Blood vessel; BW: Body weight; Cho: Total choline; $\Delta\text{Cho}/\text{H}_2\text{O}$: Change in ratio total choline to unsuppressed water; IR True FISP: Inversion recovery true fast imaging with steady state precession sequence; MoA: Mechanism of action; MRI: Magnetic resonance imaging; MRS: Magnetic resonance spectroscopy; IHC: Immunohistochemistry; PRESS: Point resolved spectroscopy; PUFA: Polyunsaturated fatty-acids; ROC: Receiver operating characteristic curve; ROI: Region of interest; T₁: Spin-lattice MR relaxation time; ΔT_1 : Change in the spin-lattice relaxation time of water protons; ΔTVol : Change in tumour volume; T/C: Treated-value divided by control-value.

Competing interests

All the authors are or were (CW) employees of Novartis Pharma AG, Basel, Switzerland. They declare no competing interests.

Authors' contributions

CW carried out the MRI and MRS studies, performed data and statistical analysis, and drafted the manuscript. PA carried out the MRI studies and critically revised the manuscript. MS performed and analysed histological and IHC studies. VR performed IHC studies and prepared figures with IHC data. SF took care of the animal model, the animal treatment, and carried out bioluminescence assessments. PM took care of the study design and coordination, performed data and statistical analysis, and drafted the manuscript. All authors read and approved the final manuscript.

Acknowledgements

We thank Caroline Fux and Mike Becquet for their excellent technical assistance, and Bettina Linssen and Barbara Zenger-Landolt from Definiens AG for helping with the Ki67 quantification. The article processing charge was funded by the German Research Foundation (DFG) and the Albert Ludwigs University Freiburg in the funding programme Open Access Publishing.

Author details

¹Oncology Research, Novartis Institutes for Biomedical Research, Basel, Switzerland. ²Global Imaging Group, Novartis Institutes for Biomedical Research, Basel, Switzerland. ³Department of Radiology Medical Physics, University Medical Center Freiburg, Magnetic Resonance Development and Application Center, Breisacher Str. 60a, 79106 Freiburg, Germany.

Received: 14 August 2013 Accepted: 11 February 2014

Published: 14 February 2014

References

1. Stephen RM, Gillies RJ: **Promise and progress for functional and molecular imaging of response to targeted therapies.** *Pharm Res* 2007, **24**(6):1172–1185.
2. Mankoff DA, Eary JF, Link JM, Muzi M, Rajendran JG, Spence AM, Krohn KA: **Tumor-specific positron emission tomography imaging in patients: [18 F] fluorodeoxyglucose and beyond.** *Clin Cancer Res* 2007, **13**(12):3460–3469.
3. Ferretti S, Allegrini PR, O'Reilly T, Schnell C, Stumm M, Wartmann M, Wood J, McSheehy PM: **Patupilone induced vascular disruption in orthotopic rodent tumor models detected by magnetic resonance imaging and interstitial fluid pressure.** *Clin Cancer Res* 2005, **11**(21):7773–7784.
4. Ferretti S, Allegrini PR, Becquet MM, McSheehy PM: **Tumor interstitial fluid pressure as an early-response marker for anticancer therapeutics.** *Neoplasia* 2009, **11**(9):874–881.
5. McSheehy P, Allegrini P, Ametaby S, Becquet M, Ebenhan T, Honer M, Ferretti S, Lane H, Schubiger P, Schnell C, et al: **Minimally invasive biomarkers for therapy monitoring.** *Emst Schering Found Symp Proc* 2007, **4**:153–188.
6. Honer M, Ebenhan T, Allegrini PR, Ametamey SM, Becquet M, Cannet C, Lane HA, O'Reilly TM, Schubiger PA, Sticker-Jantsch M, et al: **Anti-Angiogenic/Vascular Effects of the mTOR Inhibitor Everolimus Are Not Detectable by FDG/FLT-PET.** *Transl Oncol* 2010, **3**(4):264–275.
7. McSheehy P, Weidensteiner C, Cannet C, Ferretti S, Laurent D, Ruetz S, Stumm M, Allegrini P: **Quantified tumor T1 is a generic early-response imaging biomarker for chemotherapy reflecting cell viability.** *Clin Cancer Res* 2010, **16**(1):212–225.
8. Jamin Y, Tucker ER, Poon E, Popov S, Vaughan L, Boulton JK, Webber H, Hallsworth A, Baker LC, Jones C, et al: **Evaluation of clinically translatable MR imaging biomarkers of therapeutic response in the TH-MYCN transgenic mouse model of neuroblastoma.** *Radiology* 2013, **266**:130–140.
9. O'Connor JP, Carano RA, Clamp AR, Ross J, Ho CC, Jackson A, Parker GJ, Rose CJ, Peale FV, Friesenhahn M, et al: **Quantifying antivascular effects of monoclonal antibodies to vascular endothelial growth factor: insights from imaging.** *Clin Cancer Res* 2009, **15**(21):6674–6682.
10. Hakumaki JM, Poptani H, Sandmair AM, Yla-Herttuala S, Kauppinen RA: **1H MRS detects polyunsaturated fatty acid accumulation during gene therapy of glioma: implications for the in vivo detection of apoptosis.** *Nat Med* 1999, **5**(11):1323–1327.
11. Lebwahl D, Anak O, Sahmoud T, Klimovsky J, Elmroth I, Haas T, Posluszny J, Saletan S, Berg W: **Development of everolimus, a novel oral mTOR inhibitor, across a spectrum of diseases.** *Ann N Y Acad Sci* 2013, **1291**:14–32.
12. Ebenhan T, Honer M, Ametamey SM, Schubiger PA, Becquet M, Ferretti S, Cannet C, Rausch M, McSheehy PM: **Comparison of [18 F]-tracers in various experimental tumor models by PET imaging and identification of an early response biomarker for the novel microtubule stabilizer patupilone.** *Mol Imaging Biol* 2009, **11**(5):308–321.
13. O'Reilly T, Lane HA, Wood JM, Schnell C, Littlewood-Evans A, Brueggen J, McSheehy PM: **Everolimus and PTK/ZK show synergistic growth inhibition in the orthotopic BL16/BL6 murine melanoma model.** *Cancer Chemother Pharmacol* 2011, **67**(1):193–200.
14. Scheffler K, Hennig J: **T1 quantification with inversion recovery TrueFISP.** *Magn Reson Med* 2001, **45**(4):720–723.
15. Schmitt P, Griswold MA, Jakob PM, Kotas M, Gulani V, Flentje M, Haase A: **Inversion recovery TrueFISP: quantification of T(1), T(2), and spin density.** *Magn Reson Med* 2004, **51**(4):661–667.
16. Wu J: **Statistical inference for tumor growth inhibition T/C ratio.** *J Biopharm Stat* 2010, **20**(5):954–964.
17. Lehr RG, Pong A: **ROC curve.** In *Encyclopedia of Biopharmaceutical Statistics*. New York: Marcel Dekker; 2003:884–891.
18. Fardy JM: **Evaluation of diagnostic tests.** *Methods Mol Biol* 2009, **473**:127–136.
19. Lane HA, Wood JM, McSheehy PM, Allegrini PR, Boulay A, Brueggen J, Littlewood-Evans A, Maira SM, Martiny-Baron G, Schnell CR, et al: **mTOR inhibitor RAD001 (everolimus) has antiangiogenic/vascular properties distinct from a VEGFR tyrosine kinase inhibitor.** *Clin Cancer Res* 2009, **15**(5):1612–1622.
20. O'Reilly T, McSheehy PM: **Biomarker development for the clinical activity of the mTOR inhibitor everolimus (RAD001): processes, limitations, and further proposals.** *Transl Oncol* 2010, **3**(2):65–79.
21. Braunschweiger PG, Schiffer L, Furmanski P: **The measurement of extracellular water volumes in tissues by gadolinium modification of ¹H NMR spin lattice (T1) relaxation.** *Magn Reson Imaging* 1986, **4**(4):285–291.
22. Braunschweiger PG, Schiffer L, Furmanski P: **1H-NMR relaxation times and water compartmentalization in experimental tumor models.** *Magn Reson Imaging* 1986, **4**(4):335–342.
23. Rofstad EK, Steinsland E, Kaalhus O, Chang YB, Hovik B, Lyng H: **Magnetic resonance imaging of human melanoma xenografts in vivo: proton spin-lattice and spin-spin relaxation times versus fractional tumour water content and fraction of necrotic tumour tissue.** *Int J Radiat Biol* 1994, **65**(3):387–401.
24. Jakobsen I, Kaalhus O, Lyng H, Rofstad EK: **Detection of necrosis in human tumour xenografts by proton magnetic resonance imaging.** *Br J Cancer* 1995, **71**(3):456–461.
25. Jakobsen I, Lyng H, Kaalhus O, Rofstad EK: **MRI of human tumor xenografts in vivo: proton relaxation times and extracellular tumor volume.** *Magn Reson Imaging* 1995, **13**(5):693–700.
26. Fingar DC, Blenis J: **Target of rapamycin (TOR): an integrator of nutrient and growth factor signals and coordinator of cell growth and cell cycle progression.** *Oncogene* 2004, **23**(18):3151–3171.
27. Mabuchi S, Altomare DA, Connolly DC, Klein-Szanto A, Litwin S, Hoelzle MK, Hensley HH, Hamilton TC, Testa JR: **RAD001 (Everolimus) delays tumor onset and progression in a transgenic mouse model of ovarian cancer.** *Cancer Res* 2007, **67**(6):2408–2413.
28. Manegold PC, Paringer C, Kulka U, Krimmel K, Eichhorn ME, Wilkowski R, Jauch KW, Guba M, Bruns CJ: **Antiangiogenic therapy with mammalian target of rapamycin inhibitor RAD001 (Everolimus) increases radiosensitivity in solid cancer.** *Clin Cancer Res* 2008, **14**(3):892–900.
29. Shinohara ET, Cao C, Niermann K, Mu Y, Zeng F, Hallahan DE, Lu B: **Enhanced radiation damage of tumor vasculature by mTOR inhibitors.** *Oncogene* 2005, **24**(35):5414–5422.

30. Robinson SP, Rijken PF, Howe FA, McSheehy PM, van der Sanden BP, Heerschap A, Stubbs M, van der Kogel AJ, Griffiths JR: **Tumor vascular architecture and function evaluated by non-invasive susceptibility MRI methods and immunohistochemistry.** *J Magn Reson Imaging* 2003, **17**(4):445–454.
31. Landberg G, Tan EM, Roos G: **Flow cytometric multiparameter analysis of proliferating cell nuclear antigen/cyclin and Ki-67 antigen: a new view of the cell cycle.** *Exp Cell Res* 1990, **187**(1):111–118.
32. Beresford MJ, Wilson GD, Makris A: **Measuring proliferation in breast cancer: practicalities and applications.** *Breast Cancer Res* 2006, **8**(6):216.
33. Katz-Brull R, Lavin PT, Lenkinski RE: **Clinical utility of proton magnetic resonance spectroscopy in characterizing breast lesions.** *J Natl Cancer Inst* 2002, **94**(16):1197–1203.
34. Meisamy S, Bolan PJ, Baker EH, Bliss RL, Gulbahce E, Everson LI, Nelson MT, Emory TH, Tuttle TM, Yee D, *et al*: **Neoadjuvant chemotherapy of locally advanced breast cancer: predicting response with in vivo (1)H MR spectroscopy—a pilot study at 4 T.** *Radiology* 2004, **233**(2):424–431.
35. Tozaki M, Oyama Y, Fukuma E: **Preliminary study of early response to neoadjuvant chemotherapy after the first cycle in breast cancer: comparison of 1H magnetic resonance spectroscopy with diffusion magnetic resonance imaging.** *Jpn J Radiol* 2010, **28**(2):101–109.

doi:10.1186/1471-2407-14-88

Cite this article as: Weidensteiner *et al*: Tumour T₁ changes *in vivo* are highly predictive of response to chemotherapy and reflect the number of viable tumour cells – a preclinical MR study in mice. *BMC Cancer* 2014 **14**:88.

**Submit your next manuscript to BioMed Central
and take full advantage of:**

- Convenient online submission
- Thorough peer review
- No space constraints or color figure charges
- Immediate publication on acceptance
- Inclusion in PubMed, CAS, Scopus and Google Scholar
- Research which is freely available for redistribution

Submit your manuscript at
www.biomedcentral.com/submit

