Functionalized nanoporous track-etched b-PVDF membrane electrodes for lead(II) determination by square wave anodic stripping voltammetry

Haad Bessbousse, Iris Nandhakumar, Maxime Decker, Murat Barsbay, Olivia Cuscito, Didier Lairez, Marie-Claude Clochard, Travis L Wade

To cite this version:

Haad Bessbousse, Iris Nandhakumar, Maxime Decker, Murat Barsbay, Olivia Cuscito, et al.. Functionalized nanoporous track-etched b-PVDF membrane electrodes for lead(II) determination by square wave anodic stripping voltammetry. Analytical Methods, Royal Society of Chemistry, 2011, pp.1351. <10.1039/c1ay05038a>. <hal-01128108>

HAL Id: hal-01128108
https://hal.archives-ouvertes.fr/hal-01128108

Submitted on 10 Mar 2015

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L’archive ouverte pluridisciplinaire HAL, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d’enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.
Functionalized Nanoporous Track-Etched β-PVDF Membrane Electrodes for Lead(II) determination by Square Wave Anodic Stripping Voltammetry

Haad Bessbousse, Iris Nadhakumar, Maxime Decker, Murat Barsbay, Olivia Cuscito, Didier Lairez, Marie-Claude Clochard, Travis. L. Wade

1Laboratoire des Solides Irradiés, CEA-CNRS-Ecole Polytechnique, 91128 Palaiseau France
2School of Chemistry, University of Southampton, University Road, Southampton S017 1BJ UK
3Hacettepe University, Department of Chemistry, Polymer Chemistry Division, 06800 Beytepe Ankara Turkey
4Laboratoire Léon Brillouin, CEA-CNRS UMR 12, CEA-Saclay, 91191 Gif-sur-Yvette, France

Abstract

Track-etched functionalized nanoporous β-PVDF membrane electrodes, or functionalized membrane electrodes (FME), are thin-layer cells made from track-etched, poly(acrylic acid) (PAA) functionalized nanoporous β-poly(vinylidene fluoride) (β-PVDF) membranes with thin Au films sputtered on each side as electrodes. The Au film is thin enough that the pores of the membranes are not completely covered. The PAA functionalization is specifically localized in the walls of the nanoporous β-PVDF membrane by radio grafting. The PAA is a cation exchange polymer that adsorbs metal ions, such as Pb^{2+}, from aqueous solutions thus concentrating the ions into the membrane. After a calibrated time the FME is transferred to an electrochemical cell for analysis. A negative potential is applied to the Au film of the FME for a set time to reduce the adsorbed ions onto the Au film working electrode. The other metalized side of the FME functions as a counter electrode. Finally, square-wave anodic stripping voltammetry (SW-ASV) is performed on the FME to determine the metal ion concentrations in the original solution based on calibration. The calibration curve of charge versus log concentration has a Temkin isotherm form. The FME membranes are 9 μm thick and have 40 nm diameter pores with a density of 10^{10} pores/cm^2. This high pore density provides a large capacity for ion adsorption. Au ingress in the pores during sputtering forms a random array of nanoelectrodes. Like surface modified electrodes for adsorptive stripping voltammetry, the pre-concentration step for the FME is performed at open circuit. The zero current intercept of the calibration for Pb^{2+} is 0.13 ppb (μg/L) and a detection limit of 0.050 ppb based on 3S/N from blank measurements. Voltammetry (CV) and chronoperometry (CA) were used to characterize the system. The apparent diffusion coefficient (D) for Pb^{2+} in the PAA functionalized pores was determined to be 2.44 x 10^{-7} cm^2/s and the partition coefficient (pK_M) was determined to be 3.08.

The maximum allowable levels for toxic metals in water are now set at low ppb (μg/L) levels. The maximum levels of Pb^{2+} in potable water established the European Environmental Agency (EEA) the United States Environmental Protection Agency (EPA) and

*Corresponding authors
recommendations from the World health Organisation (WHO) are 7.2, 15.0, and 10.0 ppb respectively and the goal of the United States EPA is zero. Reliable quantification of these low concentrations is difficult time consuming and expensive. Also, the analysis equipment is not portable so the samples have to be sent a centralised lab which typically involves a 24 hour turn around time, which means that pollution events can be missed, or detected too late.

Electrochemical analysis techniques, such as anodic stripping voltammetry (ASV), are generally inexpensive, rapid and portable. The electrode of choice for measuring trace levels of toxic metal ions by ASV has been the dropping mercury electrodes (DME). DMEs and mercury film electrodes are very sensitive, due to their high capacity to preconcentrate ions for analysis by electro reduction, and DMEs can measure a large range of ions. The problem with mercury is that it is unacceptable for environmental applications because of its toxicity. Also, DMEs are expensive and difficult to use. Currently, there is interest in finding replacement electrodes for the DME and mercury films.

A new industry, based on thick-film screen-printed electrodes, has evolved to exploit the growing interest in environmental sensors and to replace mercury. Screen-printed electrodes are cheap and disposable but the quoted limits of detection (LOD) are barley able to measure the required low concentration levels. Also, these quoted LODs for screen-printed electrodes can be misleading because they are based on 3S/N background measurements made in ideal laboratory environments.

There have been very impressive results for the detection of Ag⁺ and As³⁺ by ASV using electrodes that do not contain mercury with LODs as low as 0.0005 ppb for Ag⁺ and 0.005 ppb for As³⁺. Lead(II) LODs are somewhat higher on non mercury electrodes with the lowest Pb²⁺ LOD being 0.020 ppb using in situ bismuth-films on a glassy carbon electrodes modified with calixarene. Other good Pb²⁺ LODs of ~0.1 ppb have been obtained on silver rotating disks electrodes, carbon electrodes modified with poly(pyrrole-malic acid) and in situ bismuth modified gold or carbon paste electrodes. The quoted LODs for mercury free screen-printed electrodes for Pb²⁺, however, are about 0.4 ppb.

We have developed a new type of thin-layer cell for use as electrochemical sensors for voltammetric analysis, figure 1a. The new cell is based on track-etched poly(acrylic acid) (PAA) functionalized nanoporous β-poly(vinyldene fluoride) (β-PVDF) membranes with porous gold electrodes on each side that function as working and counter electrodes for voltammetry, functionalized membrane electrodes (FME). The polymer film of a FME has chemically functionalized parallel nanopore channels of uniform diameter, figure 1b. The nanopore channels are formed by heavy ion irradiation and chemical etching. The heavy ion irradiation produces damage tracks in the form of radicals from broken carbon-carbon bonds. These radicals are very stable in β-PVDF due the crystallinity of the polymer. The radical tracks are chemically etched to reveal nanopore channels and the channel diameters are proportional to the etching time. After the etching, however, there are still radicals within the pores. These remaining radicals can be reacted with different monomers, such as RCCH from acrylic acid (AA) to impart chemical functionalization to the nanopore interior without blocking the pores. The functionalized nanoporous β-PVDF membranes are then transformed into electrodes by the deposition of a thin gold or conductive layer onto the membrane surfaces to make an electrically conductive thin film. The metallic layer is thin enough (35 nm) that is does not completely cover the pores. Also, the gold partially ingresses the nanopores during the sputtering. When the FMEs are immersed in a liquid sample they can selectively absorb certain ions, such as Pb²⁺, depending on their functionalization. They can then be removed from the sample, rinsed, and placed in an electrochemical cell for ASV analysis. β-PVDF is a very durable material with chemical and mechanical properties similar to Teflon and is nontoxic.
**Figure 1.**  a) Scheme of a nanopore from a gold coated PAA functionalized radio-track etched β-PVDF membrane (FME) after absorbing Pb^{2+} ions from polluted water. The β-PVDF membrane is shown as green and the RCOO⁻ as blue represents the PAA gel that is radio grafted into the 40 nm diameter nanopores of the membrane. The 35 nm thick gold coating is shown as yellow. The grey balls represent the absorbed Pb^{2+}.  d) FESEM image of a track etched β-PVDF membrane cross-section with pore diameter of 50 nm, membrane thickness of 10µm.

**EXPERIMENTAL**

**Materials:** β-poly(vinylidene fluoride) (β-PVDF) films of 9 µm thickness were provided by PiezoTech SA. Toluene, potassium hydroxide, potassium permanganate, potassium disulfite, acrylic acid (AA), Mohr’s salt ((NH₄)₂Fe(SO₄)₂ 6H₂O), sulphuric acid, C₈H₁₇N₃ HCl (EDC), phosphate buffer saline (PBS), tBuOK (C₄H₉OK 95%) were purchased from Sigma-Aldrich. Alexa Fluor R 488 hydrazide (C₂₁H₁₅N₄NaO₁₀S₂) was purchased from Invitrogen.

**Irradiation:** Prior to the swift heavy ion irradiation β-PVDF films are toluene-extracted for 24 h. The irradiation was performed at the GANIL irradiation centre (Caen, France). Films were irradiated with Kr ions (10.37 Mev/amu, fluence 10⁷ to 10¹⁰ cm⁻²) in a He atmosphere. The irradiated films were stored at -20°C in a N₂ atmosphere until chemical etching and radio grafting.

**Chemical etching:** β-PVDF irradiated films were chemically etched using permanganate solution (0.25 M) in a highly alkaline medium (KOH, 10M) at 65°C for 30 min. After etching the membranes obtained were washed in potassium disulfite solution (15%) and deionized water.

**Radio grafting:** Etched β-PVDF films were immersed at room temperature into a radio grafting solution containing AA and Mohr’s salt (0.25%w/w) in a purgeable glass tube and then connected to a Schlenk line. After 15 min of N₂ bubbling at room temperature, the glass tube is sealed and put into a thermostated water bath at 60°C for 1 h. The radio grafted film is washed with water and then Sohxlet extracted in boiling water for 24 hours in order to extract free homopolymer. The membrane was dried at 50°C under vacuum overnight.

**Field-Emission Scanning Electron Microscopy (FESEM):** FESEM micrographs were acquired with a Hitachi S-4800 microscope.
**Infra-red spectroscopy**: FTIR spectra of PVDF were obtained with a Nicolet Magna-IR 750 spectrometer equipped with a DGTS detector. Spectra were recorded in Attenuated Total Reflexion mode (ATR) using a diamond-crystal with single reflection. Spectra were collected by cumulating 32 scans at a resolution of 2 cm$^{-1}$.

**Confocal Scanning Laser Microscopy (CSLM)**: Measurements were performed with a Leica TCS-SP2 using a Ar laser (488 nm). Samples were observed in water with a 40× dry objective of numerical aperture 0.85.

**Atomic Force Microscopy (AFM)**: AFM images were acquired by tapping mode in air on a Multimode AFM system equipped with a Nanoscope III controller.

**Solutions**: The Pb$^{2+}$ solutions were diluted from 1.000 μg/mL AAS calibration standards (Alfa Aesar) or from PbCO$_3$ powder 99% (VWR). The electrolyte for the voltammetry measurements was 0.1 M sodium acetate (Sigma-Aldrich). All solutions were made with 18 Mohm deionised water (Aquadem Veolia). 100 ml polypropylene containers (VWR) were used for dilution and analysis to avoid loss of Pb$^{2+}$ due to surface adsorption on glass.

**Connections**: The functionalized membrane was metalized by gold sputtering on both sides with a K550 gold sputter (EMITECH). Gold sputtering targets were purchased from NewMet (New Metals & Chemicals LTD). The metalized sides are then connected to 0.5 mm diameter stainless steal wires with silver paste (FERRO, CDS Electronique). The connections were water proofed with hot wax and fingernail polish. Kapton tape (3M) was used to cover the surface of the electrode for some experiments.

**Voltammetry**: The voltammetry was performed in a three-compartment electrochemical cell controlled by a PalmSens potentiostat (PalmSens) or a BiStat 3200 (Uniscan). A Ag/AgCl (3M KCl) reference electrode (METROHM) was used for all measurements.

RESULTS AND DISCUSSION

The synthesis of functionalized radio grafted β-PVDF membranes was developed at the Laboratoire des Solides Irradies. β-PVDF polymer films are first bombarded by swift heavy ions, figure 2a, and the tracks formed along the ion passage are revealed under alkaline chemical treatment, figure 2b. The obtained nanoporous polymer membranes do not need to undergo subsequent e-beam irradiation to increase radicals in the polymer bulk for submicron pore diameters. After etching times less than one hour, the radical residues within the nanopore walls were sufficient for radio grafting. A confocal laser imaging study clearly shows that the PAA is localized inside the pores, figure 2d.
Indeed, when a heavy ion crosses the PVDF film, it deposits an important quantity of energy all along the latent track. This energy per mass unit (dose) is radially distributed from the ion trajectory. The energy transferred to the electrons of the polymer atoms by ion irradiation generates: defects (cross-links, chain scissions, double bonds); the creation of new active species (radicals) and gas release. The main defects in PVDF have been established by FTIR [25-27], DSC or X-ray diffraction [28]. The rapid diffusion of radicals may be related to either individual diffusion of small radical species or cooperative modes of lone electron diffusion [29]. The radical migration, initiated by the ion dose deposition, is localized in a cylinder centred around the ion trajectory with a radius roughly equal to 1µm. EPR spectra recorded under vacuum\(^1\) show the presence of various alkyl radicals (\(R^*\)): end chain radicals (\(\text{CF}_2\text{-H}_2\text{C}^*\)) or (\(\text{CH}_2\text{-F}_2\text{C}^*\)) and middle chain radicals (\(\text{CF}_2\text{-HC}^*\cdot\text{CF}_2\)) or (\(\text{CH}_2\text{-FC}^*\cdot\text{CH}_2\)). As soon as alkyl radicals are in contact with air, they immediately combine with the oxygen to form peroxy radicals (\(\text{ROO}^*\)) which are characterized by a loss of hyperfine structure in the EPR signal. EPR signals are consequently representative of both alkyl and peroxy species whatever the accelerated particle.

Damage created by ion irradiation of a polymer film display a radial profile from the track core over micrometer distances. The chemical etching removes only a fraction of these defects when stopped at submicron pore opening. In most cases, the chemical etching annihilates the residual radicals leading to a radically inactive membrane. A remarkable property of $\beta$-PVDF is that it favours the radical stability by trapping them inside its crystalline areas\([30,31]\).

The radical loss of ion irradiated PVDF film at the etching temperature of 65°C was also studied. However, 60% of radicals are kept intact even after 150 min. The radical consumption by chemical etching leads to only 5% after 150 min. It demonstrates a non-preponderant effect in radical decay by temperature annealing in comparison to radical consumption by etching.

Figure 3 shows the evolution of the residual radical fraction and the radio-grafting versus etching time. The exponential profile of the radical distribution is clearly seen.

After up to one hour of track etching, the EPR signal base line is roughly horizontal. After two hours, the baseline was no longer horizontal due to the prolonged contact with potassium permanganate which incorporated oxygen radicals into the film. A baseline correction was then necessary to extract the EPR results. Actually, we can only measure the overall radical contribution with no discrimination between alkyl and peroxy radical fractions. As plotted in Figure 3, the overall radical fraction $x_a(t)$ displays an exponential decay with a characteristic rate of 0.055 min\(^{-1}\). The presence of a persistent non-decaying radical fraction of 17% was unexpected. Indeed, as the polymer is progressively removed by etching, a continuous
decrease of radicals should be observed. It results from a compensative effect between the removal of alkyl radicals by etching and the creation of peroxyl radicals by oxidation of the remaining alkyl radicals.

![Graph](image)

Figure 3. Decay of peroxyl radicals fraction (●) and grafting yield (○) versus etching time. The initial grafting yield value was $Y_0=8\,\text{wt}\%$. The R scale corresponds to pore radii after an etching time $t: R=0.8\times t$.

In the presence of vinyl monomers such as AA, a radical polymerization takes place by a radio grafting to specifically functionalize the nanopore walls with a polymer hydrogel. Figure 4 illustrates the AA grafting yield in track-etched PVDF membranes at various etching times. It shows that the radicals persist after etching and are concentrated on the pore walls of the PVDF membranes and are able to initiate a grafting in the presence of a vinyl monomer such as acrylic acid (AA) by radical polymerisation.
The decrease of the carboxylic acid peak at 1710 cm\(^{-1}\) from FTIR for increasing etching times also follows an exponential decay. It could be directly related to EPR results. Consequently, the radical distribution profile in a track drives the radical polymerisation.

One hour etching time corresponds to pores of 44 nm of radius. Above this value, the radio-grafting is no longer homogeneous and the degree of grafting becomes very low (< 2wt%). As alkyl radicals are well-known to be more efficient as initiators in comparison to peroxyl radicals in radio-grafting process on solid polymers, the results lead to the conclusion that after two hours of etching, alkyl radicals are no longer present.

As the radical concentration decreases with the etching time, longer grafted PAA chains are favoured when the pore size increases but, simultaneously, the density of grafted PAA chains on the pore wall surface becomes very low. For a better coverage of pore walls, it is preferable to have shorter PAA chains and a denser grafted PAA chains layer. A good compromise was to radiograft pores with radius as small as 25 nm to have sufficient radicals for a good covering of pore walls.

In Figure 5, the XPS spectrum represents the surface composition of all atoms linked to C\(_{1s}\) onto track-etched PVDF membranes before and after PAA grafting. The C\(_{1s}\) ray spectrum of the initial track-etched \(\beta\)-PVDF (Fig. 6A) displays, after peak deconvolution, two typical peaks of the same height and area for CH\(_2\) and CF\(_2\) of the PVDF at 286.5 eV and 291 eV respectively. Two additional peaks at 287.8 eV and 289 eV correspond to surface oxidation peaks. The peak present at 285 eV is due the presence of non-removable PDMS contaminant present in 9 \(\mu\)m thick \(\beta\)-PVDF. Even a 24h toluene extraction did not remove these alkyl contaminants coming from grease used during the initial extrusion process. Figure 6B displays the C\(_{1s}\) ray spectrum of PAA radiografted PVDF track-etched membrane (PVDF-g-PAA). The deconvoluted signals show not only the two peaks of PVDF but also an increase of alkyl C\(_{1s}\) contribution as well as COOH peak. This gives evidence of PAA characteristic peaks at 285eV, 285.8eV and 289 eV corresponding to CH\(_2\), CH and COOH respectively.
allowing an estimation of the PAA coverage onto the track-etched β-PVDF from peaks integrations. Only 34% of the total surface at a fluence of $10^7$ tracks per cm$^{-2}$ was covered by PAA. It confirms the heterogeneity of grafting on the PVDF-g-PAA membrane surface and it gives us supplementary proof of the specific localisation of grafted PAA inside the tracks and not on the non-irradiated part of the surface of PVDF-g-PAA membranes.

The PAA grafting yields used for the FMEs were usually 10 to 15%. Higher grafting yields resulted in pores that were mostly filled by PAA hydrogel so it was impossible to have open pores for ion adsorption after the gold sputtering. Lower grafting yields indicated that the grafting did not work probably due O$_2$ contamination from insufficient N$_2$ purging of the grafting tube or the grafting tube was not well sealed.

FESEM and AFM images indicate the nature of the radiografted PAA, figure 6. For the ungrafted membrane the pore diameter is about 40 nm, figures 3a-c, while the diameter of the PAA grafted membrane is about 30 nm, figures 3d-f, showing that about a 5 nm of PAA is grafted onto the walls of the nanopores. This further indicates that there are radicals within the pore walls and the PAA is intercalated into the β-PVDF matrix as well as the surface of the pore walls. The lighter grey areas around the pores in the FESEM image, figure 3d, indicate a higher density material which is the PAA intercalated into the β-PVDF.
Figure 6. a-c) FESEM photo, AFM image and AFM line profiles of an ungrafted \( \beta \)-PVDF membrane irradiated with a fluence of \( 1 \times 10^{10} \) ions/cm\(^2\) and 30 minutes of etching and d-f) the same membrane after PAA grafting.

To transform the functionalized membrane into an electrode, a thin (35 nm) Au film is sputtered through 0.4 cm diameter holes in a homemade aluminum mask onto each surface, figures 7 and 8a. From the FESEM micrograph in figure 7b it is clearly seen that the pores of the film remain open after sputtering, however, Au does ingress the membrane pores.\(^{25}\) The Au, which protrudes into the membrane’s pores, forms 30 nm diameter, 100 nm long nanoelectrodes. The result is a membrane of with random array of \( 10^{10} \) parallel nanoelectrodes/cm\(^2\) separated from the counter electrode by 9 \( \mu \)m long 30 nm diameter pores. After sputtering the Au film through a mask, figure 8a, a 1.5 x 0.6 cm square of membrane is cut out, figures 8b and c, and connected to stainless steel wires with silver paste. The contacts are first protected with hot wax and then fingernail polish, figure 8d.
Figure 7. a) Scheme of a 9 μm thick functionalized β-PVDF membrane (green) with a 35 nm sputtered gold film (yellow) on each side. b) FESEM photo of a 9 μm thick functionalized β-PVDF membrane with a 35 nm Au film sputtered on the surface.

Figure 8. a) Photo of a 35 nm thick gold layer sputtered on each side of the functionalized β-PVDF membrane through a mask. b) and c) Photo and scheme of a metalized membrane cut out from the large surface from photo a). d) Photo of a membrane attached to wire leads with silver paste and protected with wax and fingernail polish for connection to a potentiostat.

Before a FME is used, a cyclic voltammogram (CV) is performed in a blank solution (0.1 M sodium acetate pH 4.5), figure 9a. In spite of the fact that the gold layer on the PVDF membrane is only 35 nm thick the CV shows the typical profile of a polycrystalline Au electrode. In the CV was performed on the membrane starting at 0.0 V and ramped at a scan rate of 20 mV/second to +1.2 V where the scan was reversed until the scan was stopped at +0.2 V. The other side of the FME was the counter electrode. This configuration of the working and the counter electrodes is essentially that of a thin-layer cell.

Figure 9. a) 0.4 cm diameter Au CV in 0.1 M CH₃COONa, pH ~4.5 (scan rate = 20 mV/s). The arrows indicate the sense of the scan.
The reduction peak at 0.62 V in figure 9a is the reduction of one monolayer of Au oxide formed at potentials more positive than 0.850 V during the positive scan. Integration of this reduction peak between 0.400 and 0.800 V gives a charge of 75 μC. The charge for the oxidation of a monolayer of gold (111) is 482 μC/cm². This gives an area of 0.1556 cm², however, the visual area of the FME is 0.126 cm², 0.40 cm diameter, so the roughness factor (RF) of the electrode is 1.24. This high RF is likely due to the gold ingress in pores of the membrane during the sputtering, figures 1a and 7a. Figure 9b shows the same experiment as figure 9a except the surface of the working was covered with Kapton tape in order to limit the measured current to the gold which ingresses in the pores of the membrane. This gives a surface area of 0.00229 cm², based on the same calculation as figure 9a. If we consider that the Au inside of the pores is 30 nm diameter disks then a geometric calculation of the surface gives a surface area of 0.00879 cm² so what we have measured by the CV in figure 9b is about 25% of the disk model, however, is probably in the form of Au tubes with an outside diameter of 30 nm with an unknown internal diameter and unknown length. The obvious thing to do would be to dissolve the membrane and observe the membranes side of the gold surface as was done by Vaidyanathan et al. with polycarbonate membranes with 200 nm diameter pores. β-PVDF is, however, difficult to dissolve and 30 nm structures are still a bit of a challenge to characterize so this is an on going study.

A CV of the FME in the same solution as figure 9a with 0.025 mM Pb²⁺ added at a scan rate of 100 mV/s (curve I) shows the electrochemical behaviour for the reduction and oxidation of the Pb²⁺, figure 9b. The Pb²⁺ reduction current peak occurs at -0.054 V and the oxidation peak occurs at -0.033 V. The reduction peak current is ~14 μA and the oxidation peak current is ~9 μA. Even though the peak separation is only 0.021 V the difference in currents indicates the irreversibility of the Pb²⁺ on Au. This could be the result of alloy formation or oxidation of the deposited Pb by oxygen present in solution since no purging of the solution was performed. At a scan rate of 2 mV/s (curve II) the CV is sigmoid indicating that at long times the diffusion steady-state.

![Figure 10a) CVs of a FME in a 0.025 mM Pb²⁺ solution with 0.1 M CH₃COONa, pH ~4.5 (curve I scan rate = 100 mV/s and for curve II scan rate = 2 mV/s). b) Chronoamperometric plot of a FME in a 0.0966 mM Pb²⁺ solution with 0.1 M CH₃COONa, pH ~4.5. c) Current versus time -1/2 plot of the reduction part of the chronoamperometric plot.](image-url)
Chronoamperometry experiments were performed based on the potential window seen for the CVs in figure 10a, figure 10b. The potential was switched form +0.400 V to -0.400 V and held for 5 seconds then switched back to +0.400 V and held for 5 seconds in order to measure the diffusion limited current ($I_{\text{diff}}$), the solution concentration was 0.100 mM Pb$^{2+}$. The ratio of the oxidation current to the reduction current ($i_o/i_R$) at a given time after the potential step ranges from -0.124 to -0.030 which is much lower that predicted for a simple reversible reaction of -0.293. A plot of the current for the reduction step versus $1/t^{1/2}$ yields a straight line with a good fit for the linear regression, figure 10c.

The diffusion limiting current at a disk microelectrode (in terms of the disk radius) after a potential step can be described by equation 1.

$$I_{\text{diff}} = \pi n F D^{1/2} C_o r^2 / t^{1/2} + 4nFDC_or$$

(1)

The term $n$ is equivalent/mole for the reduction ($n = -2$ for Pb$^{2+}$, equation 5), $F$ is the Faraday constant (96485 Coulombs/equivalent), $D$ is the apparent diffusion coefficient (cm$^2$/s), $C$ is the concentration of Pb$^{2+}$ (moles/L) $r$ is the electrode radius (cm) and $t$ time (s). The first term on the right is the Cottrell equation for linear diffusion and the second term on the right describes steady-state diffusion at a disk microelectrode. At short times linear diffusion dominates the current and at long times steady-state diffusion dominates current. A very convenient graphical analysis of this behaviour at a disk microelectrode was detailed by Hepel et al. The plot of $I$ versus $t^{-1/2}$ (figure 7c) has a slope equal to $I_s \pi r^2 / D^{1/2}$ and an intercept of $\pi I_s / 4$ where $I_s$ equals the steady-state current. The intercept of the line (b) and the slope (k) can be determined from equations 2 and 3.

$$D = (br/k)^2 / \pi$$

(2)

$$C_o = \pi k^2 / 4nFbr^3$$

(3)

The slope and the intercept can be taken directly from the linear regression formula in figure 10c. The radius, $r$, was found from the area determined from figure 9b by dividing by $\pi$ and taking the square root, $r = (A/\pi)^{1/2}$. This was used since the total current is the sum of all the individual nanoelectrodes. The values determined from the plot in figure 10c for $D$ is 2.44 x 10$^{-7}$ cm$^2$/s for Pb$^{2+}$ in the nanopores and a Pb$^{2+}$ concentration, $C_o$, of 116.6 mM.

Geary et al. studied the diffusion of Pb$^{2+}$ colloidal hydrogel with and without a binding agent to complex the Pb$^{2+}$. They determined a diffusion coefficient for Pb$^{2+}$ in bulk solution of 9.45 x 10$^{-6}$ cm$^2$/s. In porous media with no Pb$^{2+}$ pore interactions (i.e. no binding agent) the diffusion coefficient was 6.72 x 10$^{-6}$ cm$^2$/s and with Pb$^{2+}$/pore interactions the value ranged from 12.60 to 2.84 x 10$^{-7}$ cm$^2$/s, depending on the Pb$^{2+}$ concentration. Our value determined for PAA grafted β-PVDF nanopores is lower than those found by Geary et al. but PAA is also a stronger binding agent than that used in the colloidal hydrogel, benzo-18-crown-6, $pK_M = 2.75$. The diffusion of Cu$^{2+}$ in 36 nm diameter nanoporous polycarbonate membranes was determined to be 0.7 x 10$^{-6}$ cm$^2$/s as opposed to the bulk value of 3.0 x 10$^{-6}$ cm$^2$/s.

During the immersion of a FME in a sample containing heavy metal ions, the membrane absorbs some of the metal cations by the PAA grafted in the nanopores of the β-PVDF membrane, equation 4. The $pK_M$ of Pb$^{2+}$ in bulk PAA is 4.0 at pH < 4.0, determined by potentiometric titrations and ion-selective electrodes. The value we determined from figure 10c and equation 3 is 3.08.

$$M^{n+} + R-\text{COO}^- \leftrightarrow R-\text{COO}^\text{M}^{n+}$$

(4)
For the electrochemical analysis the FME is connected to a potentiostat and placed at a negative potential. The negative potential reduces the absorbed metals ions that are very close to the working electrode, from the poly (acrylic acid) in the pores to their metallic state at the Au surface, equation 5.

\[
R\text{-COO}M^{n+} + n\text{e}^- \rightarrow M(\text{Au})
\]  

(5)

After the reduction, square wave anodic stripping voltammetry (SW-ASV) analysis is performed in order to oxidize the metal from the working electrode surface and measure the resulting current, equation 6.

\[
M(\text{Au}) \rightarrow M^{n+} + n\text{e}^-
\]  

(6)

The parameters for the SW-ASV analysis were a frequency of 25 Hz, step amplitude of 25 mV and a potential increment of 4 mV. The optimisation of the deposition potential, time and immersion time follows: The deposition potential was determined by immersing a FME in 50 ml of stirred 3 \(\mu\)g/L Pb\(^{2+}\) sample for 10 minutes followed by SW-ASV. The charge increases with decreasing deposition potential, figure 11a. There is, however, a local minimum at \(-0.9\) V. This is likely due to the hydrogen gas bubbles from proton reduction at the FME that could impair Pb\(^{2+}\) deposition, equation 7.

\[
2H^+ + 2\text{e}^- \rightarrow H_2(g)
\]  

(7)

Also, for potentials more negative than \(-0.8\) V there was a problem with the gold electrode adhesion due to the formation of hydrogen gas bubbles. Therefore, a deposition potential of \(-0.8\) V was used for further studies. The absorption time was determined by immersing a FMS in 50 ml of a 3 \(\mu\)g/l Pb\(^{2+}\) sample for different times followed by deposition at \(-0.8\) V, figure 11b. After 30 minutes equilibrium is established. Figure 11c shows the charge versus the deposition time. After 100 seconds a plateau is reached so a minimum deposition time of 100 seconds is used for further studies.
Figure 11. a) A plot of oxidation charge from SW-ASV scans of FMEs that were immersed in 50 ml of stirred 3 μg/L Pb²⁺ samples for 10 minutes with different deposition potentials. b) A plot of the charge versus immersion time in 50 ml of stirred 3 μg/l Pb²⁺ samples using a deposition potential of -0.8 V. c) A plot of deposition time versus charge for a membrane that been immersed in 50 ml of stirred 3 μg/L Pb²⁺ samples for 30 minutes with a deposition potential of -0.8 V.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.

Figure 12 is a plot of superimposed SW-ASV current peaks for different concentrations of Pb²⁺ along with a blank scan. Each curve was obtained using a different FME. At concentrations higher than 3 to 4 μg/L current/voltage curves do not increase much in height but become very broad. For this reason the calibration curve was plotted with the charge and not peak current.
the calibration curve so it is very sensitive to slight charge variations at low concentrations. Or the discrepancy could be due to a masking of Pb$^{2+}$ by something in the tap water or perhaps complex formation by an anion such as Cl$^{-}$ or F$^{-}$.

CONCLUSIONS

The partition coefficient, pK$_M$, is lower for the PAA functionalized β-PVDF nanopores than bulk PAA by a factor of 10. This could also be a result of the uncontrolled polymerisation of the PAA. A dense hydrogel of PAA in the nanopores might not adsorb as well as more open bulk PAA or it might be difficult for the electrodeposition to efficiently extract the adsorbed Pb$^{2+}$ from the PAA in the nanopore walls. The methods used to determine the pKM for the bulk PAA were very different were a measure of the Pb$^{2+}$ uptake from solution and was not a measure of the Pb$^{2+}$ in the PAA. The measured diffusion coefficient is constant with diffusion coefficients for Pb$^{2+}$ and Cu$^{2+}$ in nanoporous media if not lower reflecting the interaction of the Pb$^{2+}$ with the grafted PAA.

The FME is very sensitive to sub-ppb concentrations of Pb$^{2+}$. The membrane preparation is done in bulk and is very inexpensive in materials. The most expensive step is the gold metallisation. We are in the process of functionalizing the PVDF membranes with polymers other than PAA to evaluate different ion adsorption efficiencies and selectivities. Because of their versatility, the FME can be thought of as a template for electroactive polymers as ion sensors.

Problems of reproducibility are likely caused by some variations in membrane etching and in the reproducibility of the grafting yields. The Temkin isotherm indicates that the energy of adsorption of Pb$^{2+}$ is inhomogeneous in the PAA functionalized membrane so there is a need to develop techniques to improve the uniformity of the PAA polymerisation. We are currently working on improving the reproducibility of the grafting yield by studying Reverse Addition Fragmentation Transfer Polymerization inside tracks. The kinetics of the adsorption isotherm needs also to be addressed in order to understand and better optimize the adsorption.

The adsorption is done at open circuit and the SW-ASV analysis is very fast, less than 3 minutes. The ability to preconcentrate the ions at open circuit means that many samples can be collected in parallel and stored for later analysis.

REFERENCES


