

Accurate characterization of pure silicon-substituted hydroxyapatite powders synthesized by a new precipitation route

David Marchat, Maria Zymelka, Cristina Coelho, Laurent Gremillard, Lucile Joly-Pottuz, Florence Babonneau, Claude Esnouf, Jérome Chevalier, Didier Bernache-Assollant

► To cite this version:

David Marchat, Maria Zymelka, Cristina Coelho, Laurent Gremillard, Lucile Joly-Pottuz, et al.. Accurate characterization of pure silicon-substituted hydroxyapatite powders synthesized by a new precipitation route. Acta Materialia, Elsevier, 2013, 9 (6), pp.6992-7004. <10.1016/j.actbio.2013.03.011>. <hal-00835892>

HAL Id: hal-00835892 https://hal.archives-ouvertes.fr/hal-00835892

Submitted on 20 Jun2013

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers. L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.

1	Accurate characterization of pure silicon-substituted hydroxyapatite powders
2	synthesized by a new precipitation route
3	David MARCHAT ^{1*} , Maria ZYMELKA ¹ , Cristina COELHO ² , Laurent GREMILLARD ³ ,
4	Lucile JOLY-POTTUZ ³ , Florence BABONNEAU ⁴ , Claude ESNOUF ³ , Jérôme
5	CHEVALIER ³ , Didier BERNACHE-ASSOLLANT ¹
6	¹ Ecole Nationale Supérieure des Mines, CIS-EMSE, CNRS:FRE3312, F-42023 158 cours
7	Fauriel Saint-Etienne cedex 2
8	² Institut des Matériaux de Paris Centre, FR 2482, Université Pierre et Marie Curie and CNRS
9	Collège de France, 11 place Marcelin Berthelot 75005 Paris, France
10	³ Université de Lyon, INSA-Lyon, MATEIS Laboratory UMR CNRS 5510, Villeurbanne F-
11	69621, France
12	⁴ Laboratoire de Chimie de la Matière Condensée de Paris, CNRS, Université Pierre et Marie
13	Curie and CNRS, Collège de France, 11 place Marcelin Berthelot 75005 Paris, France.
14	
15	E-mail addresses : marchat@emse.fr (David Marchat)*, mzymelka@emse.fr (Maria
16	Zymelka), cristina.coelho@upmc.fr (Cristina Coelho), laurent.gremillard@insa-lyon.fr
17	(Laurent Gremillard), <u>lucile.joly-pottuz@insa-lyon.fr</u> (Lucile Joly-Pottuz),
18	florence.babonneau@upmc.fr (Florence Babonneau), claude.esnouf@insa-lyon.fr (Calude
19	Esnouf), jerome.chevalier@insa-lyon.fr (Jérôme Chevalier), bernache@emse.fr (Didier
20	Bernache-Assollant),
21	
22	*Corresponding author: Phone: 0033 (0)4 77 49 97 01, Fax: 0033 (0)4 77 49 96 94
23	Address: Ecole Nationale Supérieure des Mines, Centre Ingénieurie et Santé, 158 cours
24	Fauriel 42023 Saint-Etienne, cedex 2, France.
25	

26 Abstract

This paper presents a new aqueous precipitation method to prepare silicon-substituted 27 hydroxyapatites Ca₁₀(PO₄)_{6-v}(SiO₄)_v(OH)_{2-v}(V_{OH})_v (SiHAs) and details the characterization of 28 powders with varying Si content up to y=1.25 mol mol_{SiHA}^{-1} . X-ray diffraction (XRD), 29 transmission electron microscopy (TEM), solid-state nuclear magnetic resonance (NMR) and 30 Fourier transform infrared (FTIR) spectroscopy were used to accurately characterize samples 31 calcined at 400°C for 2 h and 1000°C for 15 h. This method allows for synthesizing 32 monophasic SiHAs with controlled stoichiometry. The theoretical maximum limit of 33 incorporation of Si into the hexagonal apatitic structure is y < 1.5. This limit depends on the 34 OH content in the channel, which is a function of the Si content, temperature and atmosphere 35 of calcination. These results, particularly those from infrared spectroscopy, express serious 36 reservations about the phase purity of SiHA powders, pellets or scaffolds prepared and 37 38 biologically evaluated in the literature. 39 40 41 42 43

- 44
- ••
- 45

Keywords: biomaterials; silicon-substituted hydroxyapatite; precipitation method, infrared
spectroscopy, NMR spectroscopy.

48

49 **1. Introduction**

According to the literature, silicon-substituted hydroxyapatite (SiHA) is a highly promising 50 material in the field of bioactive bone substitutes and bone tissue engineering. It is now well-51 established that silicon plays an important role in the early stage of cartilage and bone growth 52 [1-4]. Soluble silicon species have been shown to stimulate spontaneous calcium phosphate 53 precipitation (*i.e.* the mineral bone phase) [5] and to increase bone mineral density [6]. 54 Moreover, silicon has been reported to have a positive influence on the synthesis of type I 55 collagen by human osteoblast cells (MG-63 cell line) in vitro [7]. Thereby, it is expected that 56 silicon could enhance the hydroxyapatite (HA) bioactivity [8, 9], and silicon-substituted 57 hydroxyapatites (SiHAs) have become a subject of great interest in bone repair. The SiHA 58 structure corresponds to the substitution of phosphate ions (PO_4^{3-}) by silicate ions (SiO_4^{4-}) 59 into the HA crystal structure. Different mechanisms for charge compensation have been 60 61 suggested [8, 10, 11]. The most cited one was proposed by Gibson et al. with the creation of anionic vacancies at OH⁻ sites [8, 12]. This mechanism leads to silicon-substituted 62 hydroxyapatites with the general formula $Ca_{10}(PO_4)_{6-v}(SiO_4)_v(OH)_{2-v}(V_{OH})_v$, where y 63 64 2) and V_{OH} stands for vacancies maintaining the charge balance. The incorporation of Si into 65 the HA structure in solid solution, *i.e.* without the formation of other phases, seems to be 66 limited. However, the value and the origin of this limitation are still not known, with for 67 instance the following values: 5 wt% ($\approx 1.7 \text{ mol}_{\text{Si}} \text{ mol}_{\text{SiHA}}^{-1}$) [13-15], 4 wt% ($\approx 1.4 \text{ mol}_{\text{Si}}$ 68 mol_{SiHA}^{-1} [16, 17], 3.1 wt% ($\approx 1.1 \ mol_{Si} \ mol_{SiHA}^{-1}$) [18], 2 wt% ($\approx 0.7 \ mol_{Si} \ mol_{SiHA}^{-1}$) [11, 69 19], 1.0 wt% (0.36 mol_{si} mol_{siHA}⁻¹) [20] or 0.28 wt% (0.1 mol_{si} mol_{siHA}⁻¹) [21]. Additionally, 70 it has been suggested that the concentration of 0.8 wt% of Si ($\approx 0.28 \text{ mol}_{Si} \text{ mol}_{SiHA}^{-1}$) is 71 optimal to induce the development of important bioactivity [22-24]. A value of 2.2 wt% of Si 72 73 was also reported by Thian et al. [25]. Unfortunately, in spite of extensive studies in recent

years, these results remain heterogeneous, confusing and sometimes misleading. For instance, 74 Hing et al. revealed faster bone apposition and improved adhesion and proliferation of 75 osteoblast-like cells for SiHA compared to stoichiometric HA [23, 26], whereas Palard et al. 76 found no significant difference in the behavior of MG-63 osteoblast-like cells between pure 77 HA and SiHA pellets (three compositions: y=0.2, 0.4 and 0.6 mol_{si} mol_{siHA}⁻¹) [27]. Recent 78 critical analyses of the published results regarding SiHAs have highlighted the lack of 79 experimental evidence which could explain the real effects of Si substitution on biological 80 activity in a biological environment [28, 29]. In particular, it has been criticized that the 81 physico-chemical characterizations of SiHA bioceramics are not detailed (purity, solubility, 82 rate of incorporation of Si inside the crystal lattice, etc.). Therefore, the available data do not 83 provide sufficient information to establish the origin of the improved biological performance 84 of SiHA: (i) a direct effect of SiHA by Si release, (ii) an indirect effect of SiHA by changes in 85 86 the physico-chemical properties of HA due to Si substitution (microstructure, superficial chemistry, topography, etc.) or (iii) an effect of second phases (crystalline and/or amorphous). 87 88 According to Boanini et al., the term "ion-substituted" is quite often used without any experimental proof regarding the incorporation of ions inside the crystal lattice of calcium 89 orthophosphates [28]. The unclear bioactivity of SiHA ceramics could be explained by 90 variations in the phase composition. The first evidence for this was provided by the few 91 accurate analyses available in the literature which show that SiHA powders can contain 92 crystallized [16, 30-35] and amorphous [16, 34, 36-38] impurities. The study by Kanaya et al. 93 is representative of the characterization problems of SiHA samples [38]. Indeed, while the X-94 95 ray diffraction patterns show only the characteristic lines of the HA phase (PDF: 09-432), the ²⁹Si MAS NMR spectrum revealed that only 10% of Si was incorporated into the HA lattice; 96 the rest was on the particle surface in the form of polymeric silicate species [38]. An 97 equivalent observation was made by Gasquères et al. [16]. Most studies do not evidently show 98

the purity of their SiHA samples (powders, pellets or scaffolds) [8, 9, 19, 21-24, 26, 27, 39-99 58]. They generally provide an imprecise physico-chemical characterization with assumptions 100 based on X-ray diffraction patterns or incomplete infrared band assignment [8, 9, 19, 22, 32, 101 36, 39, 59-61]. Moreover, infrared vibrations at 692, 840, 890 and 945 cm⁻¹, detected on an 102 SiHA sample containing 1.6 wt% Si (1200°C for 2 h), were attributed without evidence by 103 Gibson et al. to the substitution of SiO_4 for PO₄ into the HA lattice [8, 12]. Unfortunately, this 104 article set the standard for SiHA analysis by infrared spectroscopy and has been widely cited 105 106 to prove the purity of SiHA powders synthesized using Gibson's method [9, 23, 39, 40, 43, 44, 46, 47, 53, 57] or displaying the same new infrared bands [14, 32, 36, 48, 50, 54, 62]. 107

Several methods are used to prepare Si-substituted hydroxyapatites (SiHAs), such as 108 the sol-gel route [48], resuspension processes [20, 33, 34, 63-66], solid state reactions [10, 109 67], hydrothermal techniques [17, 68, 69], mechanochemical methods [70], magnetron 110 111 sputtering [14], pulsed laser deposition [51, 71], electrophoretic deposition [72] and precipitation from aqueous solutions. Aqueous precipitation methods are the most often 112 113 described and set up in the literature. Two different procedures are used to produce Si-HA 114 from aqueous solutions: (i) the acid-base neutralization [8, 9, 16, 19, 23, 30, 35, 37, 39, 46, 47, 49, 50, 53, 56, 57, 73-75], and (ii) the use of phosphorus and calcium salts [13, 21, 32, 36, 115 37, 60, 74, 76, 77]. Generally, far less attention has been devoted to the silicon reagent. Two 116 organic compounds are mainly used as a source of silicate ions: tetraethylorthsilicate (TEOS, 117 $Si(OC_2H_5)_4$) and tetraacetoxysilane (TAS, $Si(COOCH_3)_4$) which are not miscible in water. 118 Powders synthesized through these methods are poorly crystallized and often contaminated by 119 second phases (e.g. α and β -Tricalcium phosphate, amorphous phase, silicocarnotite [16, 19, 120 30, 31, 36-38, 49, 59, 60, 63, 64, 67, 74, 76]) or undesired ions like Mg [56], S [77] or Na [78, 121 79]. 122

In order to correctly describe the physical, chemical and biological properties of 123 SiHAs and to compare them to routinely implanted HA and β -TCP, well-characterized pure 124 SiHAs powders first need to be prepared. Therefore, this work was devoted to the 125 development of a new route to synthesize monophasic SiHA powders with controlled 126 stoichiometry. To this purpose, a solution of soluble silicate was first prepared from TEOS via 127 a sol-gel route, and then accurate powder analysis was carried out by means of ICP/AES, X-128 ray powder diffraction, Rietveld refinement, high resolution electron transmission microscopy 129 (HR-TEM) with energy dispersive spectroscopy (EDS) as well as infrared (FT-IR/ATR) and 130 solid-state NMR spectroscopy. Two pH levels of precipitation were studied, as well as six 131 Si/P molar ratios. 132

133 2. Materials and methods

134 **2.1 Powder synthesis**

HA and SiHA powders were prepared through an aqueous precipitation method using a fully 135 automated apparatus. A diammonium hydrogen phosphate aqueous solution ((NH₄)₂HPO₄, 136 137 99%, Merck, Germany), and, if applicable, an alkaline silicate solution were added to a calcium nitrate solution (Ca(NO₃)₂, 4H₂O, 99%, Merck, Germany) using peristaltic pumps. 138 The reaction was performed under an argon flow (4.8, AirLiquide) to prevent any excessive 139 carbonation of precipitates. The pH of the suspension was adjusted by the addition of a 28% 140 ammonia solution (Merck, Germany) by means of a pH stat (Hanna Instruments), and the 141 temperature was controlled and regulated automatically with an external T-probe. The 142 suspension was continuously stirred and refluxed. After complete introduction of the 143 solutions, the suspension was matured for 24 h, and then filtered under vacuum. Finally, the 144 precipitates were dried at 70°C overnight. 145

The solution of soluble silicates was prepared from tetraethylorthosilicate (TEOS
≥99%, Aldrich, Germany) *via* a sol-gel route. The original step consisted of the preparation of

a silica gel through the hydrolysis and condensation of this precursor. First, the alkoxide 148 groups (Si-OEt) of TEOS were hydrolyzed to silanol groups (Si-OH). The reaction was 149 catalyzed by a nitric acid aqueous solution (7.5 10^{-3} M). This generates a considerable amount 150 of monomers (Si-OH), which aggregate and form a colloidal suspension called the "sol". This 151 reaction, based on Klein et al. [80], was carried out by maintaining the molar ratio of 152 TEOS/ethanol/acidified water at 1.0/8.5/4.0 and the solution at 25°C in an ambient 153 atmosphere. Second, the condensation of the silanol or alkoxide groups was initiated by 154 increasing the solution pH to a basic level, about pH 8, with a few drops of pure 28% 155 ammonia solution (Merck, Germany). This reaction creates siloxane bridges (Si-O-Si), 156 leading to the formation of a silica gel. The gelation reaction was continued for about 12 h at 157 25°C. Finally, a solution of soluble silicates was obtained by depolymerization of the silica 158 gel. This was achieved through the nucleophilic attack of siloxane linkages (Si-O) by 159 160 hydroxide ions in pure 28% ammonia solution (pH > 11). After filtration through a Millipore filtration unit (Magma nylon, 0.8 µm), the soluble silicate ion concentration of these solutions 161 was measured by means of an ion-exchange chromatography system (DIONEX DX-500) 162 equipped with a SiO_4^{4-} ion exchange column (AS4A) with a UV/Vis detector (410 nm). The 163 soluble silicate ion concentration in these solutions was, on average, 1076 ± 34 ppm (n=14 164 solutions). This value is a function of the preparation process (e.g. hydrolysis, condensation 165 and depolymerization reactions). Thereby, the volume of the solutions of soluble silicates was 166 adjusted for each synthesis. 167

168 A pure HA powder $Ca_{10}(PO_4)_6(OH)_2$ was first prepared to be used as a reference 169 material for further SiHA syntheses and analyses. This was obtained at a pH and temperature 170 of precipitation of 9.5 and 50°C, respectively, with a maturation time of 24 h, and a reagent 171 (Ca/P) molar ratio equal to 10/6.

The reagent ratios used to prepare the SiHA powders were calculated by assuming, 172 first, the general formula $Ca_{10}(PO_4)_{6-v}(SiO_4)_v(OH)_{2-v}(V_{OH})_v$ and, second, a constant molar 173 ratio Ca/(P+Si) equal to 10/6. The volume of the calcium and phosphate aqueous solutions 174 was fixed at 500 mL and 250 mL, respectively. Table 1 summarizes the amount (mol) of Ca, 175 P and Si used for each (Si)HA powder prepared with y equal to 0, 0.25, 0.50, 0.75, 1.00, 1.25; 176 designated hereafter as HA, Si_{0.25}HA, Si_{0.50}HA, Si_{0.75}HA, Si_{1.00}HA and Si_{1.25}HA, respectively. 177 Precipitations were achieved at 50°C for 24 h of maturation time, according to the preliminary 178 tests performed on pure HA. Two parameters of precipitation were examined, the pH of 179 precipitation and the stoichiometric number y, *i.e.*, the amount of silicate theoretically 180 incorporated into the apatite structure. Precipitations were conducted either at pH 9.5, 181 previously established for HA synthesis, or at pH 10.80 \pm 0.05. The former was chosen 182 according to phosphate and silicate speciation curves, in order to have HPO₄²⁻ [81] and 183 184 H_3SiO_4 ions [82] in solution as the main phosphate and silicate species, respectively. The studied parameters are listed in Table 1. 185

The as-synthesized powders were heated under air using an alumina crucible. Aliquots of each sample were calcined both at 400°C for 2 h (designated hereafter as "raw powders"), in order to remove synthesis residues, and at 1000°C for 15 h under air according to ISO norm 13779-3 in order to characterize powders with a well-defined structure. The heating and cooling rate was fixed at 4°C min⁻¹.

191 **2.2 Powder characterization**

192 2.2.1 X-ray powder diffraction and Rietveld refinement

193 Crystalline phases were identified by means of a Siemens D5000 $\theta/2\theta$ X-ray diffractometer 194 (XRD) using CuK α radiation and operating at 40 kV and 20 mA. XRD patterns were first 195 collected over the 2 θ range of 10-60° at a step size of 0.03° and counting time of 4 s per step 196 in order to determine the phase composition. Crystalline phases detected in the patterns were

identified by comparison to standard patterns from the ICDD-PDF (International Center for 197 Diffraction Data-Powder Diffraction Files). In addition, high resolution XRD scans were 198 obtained on calcined powders from 10° to 120° in 0.02° steps with a counting time of 10.5 s 199 per step. These patterns were used to calculate the lattice parameters and the crystalline size 200 by full pattern matching. In this mode, the positions of the diffraction peaks and the 201 systematic extinctions are calculated from the cell parameters and the space group. The 202 intensities of the lines are adjusted by the refinement program and not calculated from the 203 204 atomic positions. The refinements were performed using the space group of the HA structure P63/m (PDF 09-432) by means of the Topas software (Bruker, Germany). The initial cell 205 parameters were taken as a = 9.42Å and c = 6.88Å. 206

The evolution of the crystallinity of the samples after calcination at 1000°C for 15 h was evaluated by means of the full width at half maximum (FWHM) of the (211) peak at $2\theta=31.8^{\circ}$, as it had the highest intensity and minimal overlap with neighboring peaks.

210 **2.2.2 Infrared spectroscopy**

Fourier transform infrared (FT-IR) measurements were carried out with the use of a MIR TF VERTEX 70 Spectrometer by means of the ATR system. The spectra were recorded over the range of 450-4000 cm⁻¹ with a resolution of 2 cm⁻¹. Spectra were obtained by signal averaging 32 successive scans. Every measurement was at least duplicated on two independent powder samples crushed by hand, with an agate pestle and mortar, and deposited on the ATR system. Spectra were normalized with respect to the v_4 band of the phosphate group at about 602 cm⁻¹, according to a classical procedure [83, 84].

218 **2.2.3 NMR spectroscopy**

NMR spectra were recorded on a Bruker AVANCE 300 spectrometer: $B_0 = 7.05$ T, $v_0(^{1}H) = 300.13$ MHz, $v_0(^{31}P) = 121.49$ MHz, $v_0(^{29}Si) = 59.62$ MHz, using a CP-MAS Bruker probe with 4 mm rotors spinning at 14 kHz for ¹H and ³¹P and with 7 mm rotors spinning at 5 kHz for ²⁹Si. Chemical shifts are referenced to TMS for ¹H and ²⁹Si and 85% aqueous H₃PO₄
for ³¹P. Single pulse and CP (cross-polarization) MAS experiments have been used to study
these materials. CP MAS relies on the heteronuclear dipolar interaction between an abundant
spin X (¹H here) and a low abundant nuclei Y (³¹P and ²⁹Si here). It allows the study of local
molecular motion. The NMR parameters are summarized in Table 2.

227 **2.2.4 Electron microscopy (HR-TEM, SAED and EDX)**

High resolution transmission electron microscopy (HR-TEM) was conducted on calcined 228 powders (1000°C/15 h) using a JEOL 2010 F Microscope at a voltage of 200 kV. Samples 229 were prepared by dispersing the powders in ethanol. After sonication at 40 W for 5 min, a 230 small drop of the suspension was placed onto copper mesh grids coated with a holey carbon 231 film. Finally, a thin coating of gold (10 nm in thickness) was sputtered on half of the grid. 232 Gold was then distributed as crystallized nano-domains which were used as a reference in the 233 234 selected area electron diffraction (SAED) patterns to calculate as precisely as possible the lattice parameters. The SAED patterns obtained from regions with or without gold on the HA 235 236 part were the same.

237 **2.2.5 Elemental analysis**

The silicon, phosphorous and calcium content in powders was determined by inductively 238 coupled plasma atomic emission spectrometry (ICP/AES) (HORIBA Spectrometer, Jobin-239 Yvon, Activa model). Powder samples were dissolved in a nitric acid solution (0.5 M). 240 Solutions were prepared (e.g. powder mass, dilution) in order to limit the measurement 241 uncertainty as well as to determine the concentrations of Ca, P and Si within the highest 242 sensitivity range of the ICP/AES device (around 30 ppm). Lastly, the carbon content in the 243 powders was determined using an elemental analyzer with an infrared detector (LECO CS-244 444 carbon and sulfur analyzer). 245

The stoichiometric number <u>y</u> was determined by means of Eq. 4, assuming that powders containing $0 \le wt\%$ Si ≤ 2.81 (or $0 \le y \le 1.00$) are pure monophasic SiHAs Ca₁₀(PO₄)_{6-v}(SiO₄)_v(OH)_{2-v}(V_{OH})_v, without any second crystalline or amorphous phase.

249 % wt Si =
$$(m_{Si} 100 / m_{SiyHA}) = (Cm_{Si} V_{sol} 100) / (m_{SiyHA})$$
 (1)

250
$$n_{Si} = (\% \text{ wtSi } m_{SiyHA}) / (M_{Si} \ 100)$$
 (2)

251
$$M_{SiyHA} = M_{HA} - (19.895 y_{Si})$$
 (3)

252
$$y_{Si} = (n_{Si} M_{SiyHA}) / (m_{SiyHA}) = (\% wtSi M_{HA}) / (100 M_{Si} + 19.985 \% wtSi)$$
 (4)

where % wt Si is the mass percentage of Si in the powder, Cm_{Si} is the mass concentration of Si in the analyzed solution by ICP/AES (ppm or mg L⁻¹), V_{sol} is the volume of the analyzed solution (L), m_{SiyHA} is the mass of the powder dissolved in the former solution (mg), and M_{SivHA} , M_{HA} and M_{Si} are the molar masses of SiyHA, HA and Si, respectively (g mol⁻¹).

3. Results and discussion

258 3.1 Influence of pH on the SiHA phase composition

259 Si_{0.50}HA powders were synthesized at 50°C with pH values equal to 9.50 (Si_{0.50}HA-9.5) and 10.80 (Si_{0.50}HA-10.8). Fig. 1 shows the XRD diffractograms of powders calcined at 1000°C 260 for 15 h. The pattern of the Si_{0.50}HA-9.5 sample presents two different crystalline phases 261 matching the ICDD standard for hydroxyapatite (HA, PDF 9-432) and α -tricalcium phosphate 262 (α -TCP, PDF 9-348). The Si_{0.50}HA-10.8 diffractogram displays only the characteristic 263 diffraction lines of HA. This result indicates that the final composition of the powders is a 264 function of silicate ion speciation. H₃SiO₄ or more basic forms of silicate ions have to be 265 maintained during the synthesis to obtain a thermally stable SiHA phase, *i.e.* a monophasic 266 267 powder after heat treatment at 1000°C/15 h. Therefore, herein, the following results are presented for powders prepared at pH 10.8. Under these synthesis conditions, the general 268 269 reaction of precipitation can be written as follows:

270
$$10Ca^{2+}+(6-y)HPO_4^{2-}+yH_3SiO_4^{-}+(8+y)OH^{-} \leftrightarrow Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-y}(V_{OH})_y +(6+2y)H_2O$$
 (5)
11

To our knowledge, this is the first time that a true precipitation reaction has been given forSiHA.

273 **3.2 Influence of the Si content** (y_{Si})

274 **3.2.1 X-ray diffraction analysis**

Fig. 2 shows the diffraction patterns of HA and Si_vHA ($y_{Si} = 0.25, 0.50, 0.75, 1.00$ and 1.25 275 mol) raw powders. Each pattern matches well with the standard pattern of HA (PDF 9-432). 276 No other phase was detected. The samples exhibit broad diffraction lines which indicate very 277 small crystallites and/or low crystallinity. More, the FWHM increased with silicon content. 278 The diffractograms of heat treated powders (1000°C/15 h) are displayed in Fig. 3. They 279 present no secondary phase besides hydroxyapatite for a silicon content up to $y_{Si} = 1.00$. On 280 the other hand, HA (PDF 9-432) and α -TCP (PDF 9-348) were detected in the pattern of 281 Si_{1.25}HA calcined at 1000°C for 15 h. Moreover, as observed for the raw powders, the 282 283 crystallinity of Si_vHA calcined powders with $1 \ge y \ge 0$ decreased with an increase in the silicate content. Indeed, the higher the Si content, the higher the FWHM of the diffraction 284 line. For instance, the FWHM of the diffraction line at 31.8° (20) increased as follow: 0.070 285 $(HA) < 0.096 (Si_{0.25}HA) < 0.160 (Si_{0.50}HA) < 0.164 (Si_{0.75}HA) < 0.170 (Si_{1.00}HA)$. This is due 286 to both direct (decrease in the crystallinity) and indirect (decrease in the crystallite size) 287 effects of Si, but the individual contributions of these effects cannot be evaluated by X-ray 288 diffraction. 289

The XRD patterns indicate that whatever the amount of silicon ranging between $0 \le$ wt%Si \le 3.51 (or $0 \le y \le 1.25$), the crystalline phase of the precipitates is a hydroxyapatite (PDF 09-432). Thereby, silicon can be incorporated in the apatitic structure, or in an amorphous phase or in both phases. However, only precipitates containing up to 2.81 wt%Si (or y = 1.00) are thermally stable at 1000°C for 15 h.

295 **3.2.2 Lattice parameter refinement**

Refinement was performed on monophased heat-treated powders ($0 \le y \le 1.00$). The results, displayed in Table 3, reveal changes in the apatitic structure parameters. The Si substitution causes *c*-axis and unit cell volume expansion as well as a reduction in the mean crystallite size. The same observation was reported in other studies [10, 17, 32, 70, 85]. On the other hand, and in contrast to the linear increase of the lattice parameter *c* with an increasing amount of Si, the *a* lattice parameter fluctuates at random between 9.416 Å and 9.428 Å. These results highlight that all or part of the silicon is incorporated into the apatitic structure.

303 **3.2.3 Elemental analysis**

The experimental Ca/(P+Si) molar ratios of the final calcined powders are presented in Table 1. Values are in accordance with the expected ones (1.67) for all compositions, considering experimental error. Moreover, the calcined powders were not carbonated since the carbon content by weight was equal to 0.03, 0.07, 0.05, 0.05 and 0.05 wt% (\pm 0.02 wt%) for HA, Si_{0.25}HA, Si_{0.50}HA, Si_{0.75}HA and Si_{1.00}HA, respectively.

The results, presented in Table 1, show that the chemical formulas of SiHA calculated first by the measured silicon contents, then by the the theoretical formula $Ca_{10}(PO_4)_{6-}$ $_{v}(SiO_4)_{v}(OH)_{2-v}(V_{OH})_{v}$ and finally using Eq. 4 are in a good agreement with the nominal ones.

312 **3.2.4 Electron microscopy**

A low magnification bright-field image of heat-treated $Si_{1,00}$ HA particles is shown in Fig. 4a. 313 SiHA powders are composed of round particles, smaller than 100 nm in diameter for 314 Si₁₀₀HA, whereas the HA powder shows bigger acicular crystals [86]. At higher 315 magnification, grains do not present any dislocation or disorder within the central region. 316 Similarly, high-resolution lattice images of the grain surface do not show any amorphous or 317 disordered layer (see Fig. 4b). A selected area electron diffraction (SAED) pattern obtained on 318 the same grain is displayed in Fig. 5a. SAED patterns show a diffraction pattern with well-319 defined spots regardless of the selected area. This indicates the high crystallinity of the heat-320

treated SiHA powders and the homogeneity of the crystals. Second, a very good agreement 321 appears between the SAED patterns and the PDF card 09-432 of HA as identified by X-ray 322 diffraction. Moreover, no halo ring was observed, confirming the absence of the amorphous 323 phase. Fig. 5b shows a SAED pattern for the [010] zone axis. Two other SAED patterns were 324 obtained for the [1-10] zone axis. Indexation of these patterns allows for calculating the c/a325 ratio by means of the interval between two spots. Thus, for instance, according to the 326 hexagonal crystallographic structure identified by X-ray diffraction and the distance D_1 and 327 D_2 between two spots along the [h00] and [001] directions ([010] zone axis, Fig. 5b), 328 respectively, the c/a ratio was calculated as follows: 329

330
$$(c/a)^2 = \frac{3}{4} (D_1/D_2)^2$$
 (6)

The results are the average of about ten intervals per pattern. A c/a ratio of 0.730 ± 0.005 was determined. Moreover, other experimental patterns for different zone axes (not shown here) were obtained and compared to theoretical electron diffraction patterns calculated by means of the Java Electron Microscopy Simulation (JEMS) software [87]. The results indicate that the experimental and simulated patterns are perfectly superimposed for 0.734 \ge c/a \ge 0.729. Additionally, the c/a ratio value from PDF 09-432 (0.7309) is included in this range.

338 3.2.5. Solid-state NMR analysis

339 **3.2.5.1.** ³¹P MAS NMR

The ³¹P MAS NMR spectra of HA, Si_{0.50}HA and Si_{1.00}HA calcined at 1000°C for 15 h are shown in Fig. 6a. The spectra present a main narrow peak which corresponds to the single P site of hydroxyapatite [88], and whose position shifts to higher frequencies with increasing silicon content: 2.8 ppm for HA, 3.0 ppm for Si_{0.50}HA, and 3.1 ppm for Si_{1.00}HA. Likewise, the FWHM broadens: 166 Hz < 188 Hz < 233 Hz for raw HA, Si_{0.50}HA and Si_{1.00}HA, respectively (figure not included), and 55 Hz < 132 Hz < 233 Hz for calcined HA, Si_{0.50}HA

and $Si_{1,00}HA$, respectively (Fig. 6a). The chemical shift and peak broadening indicate that the 346 SiHA structure is different from a perfect hydroxyapatite short-range structure. The increasing 347 line width suggests an increase in local disorder around those phosphate groups where Si is 348 incorporated in the HA structure. Besides the 2.8 ppm peak, two additional weak broad peaks 349 at 4.6 and 5.8 ppm were detected in the ³¹P spectra. The peak at 4.6 ppm was only revealed in 350 the ${}^{1}\text{H} \rightarrow {}^{31}\text{P}$ CP MAS spectrum (Fig. 7b). HA powder did not present the 4.6 ppm signal (Fig. 351 7a). According to Hartmann et al. [89], the ³¹P MAS peak at 5.8 ppm corresponds to PO₄ 352 tetrahedra in a proton-free region of a hydroxyapatite channel structure containing OH 353 vacancies (i.e. along the crystallographic c-axis). These proton-free regions, observed in 354 oxyhydroxyapatite $Ca_{10}(PO_4)_6(OH)_{2-2x}(O)_x(V_{OH})_x$ (OHA), must exist in silicon-substituted 355 $Ca_{10}(PO_4)_{6-v}(SiO_4)_v(OH)_{2-v}(V_{OH})_v$ (SiHA), hydroxyapatite silicon-substituted 356 or oxyhydroxyapatite $Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-y-2x}O_x(V_{OH})_{x+y}$ (SiOHA). The assignment of the 357 peak at 4.6 ppm, that seems related to the incorporation of Si in the apatite lattice, will be 358 discussed later on (section 3.2.5.3). 359

360 **3.2.5.2.** ¹H MAS NMR

The ¹H MAS NMR spectra of pure HA, Si_{0.50}HA and Si_{1.00}HA powders calcined at 1000°C 361 for 15 h are shown in Fig. 6b. Two signals were observed, one sharp at 0 ppm and one 362 broader at about 5.2 ppm. The former (0 ppm) is characteristic of OH groups in crystalline 363 HA [89]. Moreover, and similarly to the ³¹P signal at 2.8 ppm, the greater the Si content in the 364 apatitic structure of the calcined powders, the broader the FWHM of the signal at 0 ppm 365 (FWHM = 108 Hz for HA, 191 Hz for Si_{0.5}HA and 228 Hz for Si_{1.00}HA). This suggests a 366 change in the environment around the hydroxyl groups, highlighting the modification of O-H 367 bond distances due to Si. As postulated by Gomes et al., this concomitant broadening of the 368 ³¹P and ¹H resonances with Si content confirms the incorporation of Si atoms into the apatite 369 lattice [30]. The signal at 5.2 ppm was attributed by Hartmann et al. to OH⁻ positions missing 370

only one neighboring ion in OHA channels [89]. This type of OH⁻ group along the channels of the apatite structure leads to the formation of "proton pairs" stabilized by a hydrogen bond. The intensity of this proton position is higher in SiHA samples than in HA, but does not seem to be an exclusive function of the Si content (see Fig. 6b). Therefore, ¹H MAS NMR indicates the presence of two types of OH⁻ groups along the channels of the apatite structure: an unchanged proton line position with continuous OH⁻ groups (0 ppm) and OH⁻ pairs surrounded by vacancies (5.2 ppm).

378 **3.2.5.3.** ¹H-³¹P HETCOR CP MAS

To confirm that the entire proton position is located in the apatite channel structure, two-379 dimensional ¹H-³¹P HETCOR CP MAS experiments were performed on raw and calcined 380 powders. Fig. 8 presents ¹H-³¹P HETCOR CP MAS spectra recorded on raw Si₁₀₀HA (Fig. 381 8a) and calcined $Si_{0.50}$ HA (Fig. 8b) powders. The spectra show two main 2D correlation peaks 382 on both raw and calcined powders. The same peaks were observed for Si_{0.25}HA, Si_{0.50}HA and 383 Si_{1.00}HA (HETCOR CP MAS results for calcined Si_{0.25}HA and Si_{1.00}HA not included). The 384 385 stronger one (peak A, Fig. 8b), characteristic of an ideal HA structure, is due to the dipolar interaction between the P sites ($\delta(^{31}P) = 2.8$ ppm) and the OH sites ($\delta(^{1}H) = 0$ ppm). It 386 corresponds to an undisturbed hydroxyapatite short-range structure [89]. The second one 387 (peak B, Fig. 8b) appears between the ³¹P signal at 4.6 ppm and the ¹H signal at 5.2 ppm. Its 388 intensity increases with heat treatment (Fig. 8) and the Si content (data not included). This 389 390 correlation is not observed for the HA sample (data not included). Moreover, a low extent of peak B is observed with the main ³¹P peak at 2.8 ppm (peak C, Fig. 8b). The intensity of this 391 2D correlation peak becomes stronger with Si content as well. More generally, the higher the 392 393 amount of Si incorporated into the SiHA structure, the stronger the dispersion of the main correlation between A and B along the ³¹P axis. Finally, as expected, the HETCOR spectra 394 show no correlation peak of the ³¹P line at 5.8 ppm, confirming that it corresponds to a 395

proton-free phosphate position. To conclude, first the broadening of peak A indicates an 396 increase in the distribution of P-H bond distances when silicate is incorporated into the HA 397 structure, corresponding to the loss of local ordering in the phosphate environment. Second, 398 peaks B and C correspond to two distinct P sites in the vicinity of isolated pairs of protons 399 (OH⁻ pairs) present in the channel structure of silicon-substituted oxyhydroxyapatite 400 $Ca_{10}(PO_4)_{6-v}(SiO_4)_v(OH)_{2-v-2x}O_x(V_{OH})_{v+x}$ (SiOHA): (i) peak B represents a very strongly 401 distorted hydroxyapatite short-range structure and (ii) peak C represents a less distorted one. 402 Peak B is clearly related to SiO₄ substitution and proves once again that charge compensation 403 implies OH vacancies along the channels, leading to the formation of OH⁻ pairs in the vicinity 404 of the substituted PO₄ tetrahedra. Peak C can be due to SiO₄ substitution as well as 405 dehydration of SiHA, both leading to the formation of OH vacancies in SiOHA. 406

407 **3.2.5.4.** ²⁹Si MAS NMR

The ²⁹Si MAS NMR spectra of Si_{1.00}HA powders, raw and calcined, are shown in Fig. 9. The 408 raw powders present two resonances: one sharp at about -72 ppm that is clearly attributed to 409 $SiO_4^{4-}(Q^0)$ in the apatitic structure [90], and a broad peak at about -100/-110 ppm which 410 corresponds to Q^3/Q^4 silicon species [16]. The results confirm that the main part of the silicate 411 is incorporated into the HA lattice during precipitation, according to the main reaction Eq. 1. 412 The rest of the silicates are adsorbed at the crystallite surface, as observed for phosphates 413 during the precipitation of apatitic calcium phosphates [91, 92]. After calcination, the broad 414 peak at -100/-110 ppm disappears without the detection of new signals, similar to those 415 reported in the literature (Si-TCP or α -Ca₃Si₃O₉) [16, 30, 38]. The same results were obtained 416 for the $Si_{0.25}$ HA and $Si_{0.50}$ HA samples (data not included). 417

- 418 **3.2.6. FT-IR analysis**
- 419 3.2.6.1 As-synthesized samples

The IR spectra of the raw HA and SiHA powders with a silicon content up to $y_{Si} = 1.25$ mol 420 (figure not included) present strong similarities and exhibit intense bands characteristic of 421 hydroxyapatite. They correspond to the four vibrational modes of phosphate groups (v_1 , v_2 , v_3 , 422 and v_4), and the stretching (v_s) and librational (v_L) modes of the hydroxide groups [81, 92-94]. 423 The intensity of the latter, at 630 cm⁻¹ (v_L) and 3570 cm⁻¹ (v_S), clearly decreased with the 424 amount of silicon. These results confirm that the as-synthesized precipitates exhibit the 425 hydroxyapatite phase, regardless of the amount of silicon ranging between $0 \le wt\%$ Si ≤ 3.51 426 (or $0 \le y \le 1.25$), as observed on the diffractograms (Fig. 2). A more accurate description of 427 the infrared spectra of the as-synthesized SiHA powders is available in a complementary 428 article [95]. 429

430 **3.2.6.2** Calcined samples – general observations

Fig. 10 compares the infrared spectra of heat-treated HA and SiHA powders (1000°C/15 h). 431 432 The HA and Si_yHA with $0 \le y \le 1.0$ powders mainly present bands characteristic of hydroxyapatite with the v_1 (962 cm⁻¹), v_2 (473 cm⁻¹), v_3 (1021 and 1085 cm⁻¹) and v_4 (562 and 433 600 cm^{-1}) modes of PO₄³⁻, as well as the stretching (v_S: 3572 cm⁻¹) and librational (v_L: 629 cm⁻¹) 434 ¹) modes of hydroxide groups [81, 92, 94]. A shoulder at 947 cm⁻¹ was also observed for HA 435 and SiHA powders. The relative intensity of this shoulder was slightly higher for SiHA than 436 for HA, but did not seem to be a function of the amount of Si. Besides the low hydroxyapatite 437 vibrations, the spectrum of the Si_{1.25}HA powder presents mainly the characteristic bands of α -438 TCP and traces of β -tricalcium phosphates (β -TCP): the weak band at 495 cm⁻¹ ascribed to 439 the O-P-O v_2 vibrational mode of β -TCP, the bands due to the splitting of the v_4 mode at 567 440 cm^{-1} in α -TCP (551, 560, 580, 595 and 611 cm^{-1}), the bands at 945 and 955 cm^{-1} assigned to 441 the degenerated symmetric P-O stretching vibration of the phosphate ions (v_1) in β - and α -442 TCP, respectively, and the bands corresponding to the strong asymmetric P-O stretching 443 mode (v₃) for β -TCP (988, 1025 cm⁻¹) and α -TCP (988, 1013, 1025, 1031 and 1055 cm⁻¹) [52, 444 18

445 96]. This result is complementary to the X-ray diffraction pattern (Fig. 3) and indicates that
446 the Si_{1.25}HA apatitic precipitate decomposes during heat treatment with the formation of TCP
447 and amorphous silica species.

448 3.2.6.3. Calcined samples – accurate IR band assignment of the pure SiHA phase

As opposed to HA, the FT-IR spectra of the calcined Si_vHA powders, with $0 \le y \le 0.75$, 449 exhibit nine new bands or shoulders (sh) at 491 (sh), 504, 528, 750, 840, 893, 930 (sh), 985 450 (sh) and 1002 (sh) cm⁻¹. The intensity of these new vibrations increased with the amount of 451 Si, except for the weak band at 840 cm⁻¹ and the shoulder at 930 cm⁻¹ which remained 452 relatively constant. Conversely, the intensity of the absorption bands attributed to the four 453 vibrational modes of PO_4^{3-} and both modes of OH^- in hydroxyapatite decreased as the amount 454 of Si increased in the range $0 \le y \le 1.00$ (e.g. v_S OH : 0.49 (HA) > 0.39 (Si_{0.25}HA) > 0.35 455 $(Si_{0.50}HA) > 0.12$ $(Si_{0.75}HA) > 0.07$ $(Si_{1.00}HA)$). More precisely, the v_L mode decreased to the 456 457 detection limit for y = 1, while the stretching the OH⁻ band decreased and broadened. In fact, two new vibrations at 3565 and 3552 cm⁻¹, close to the main one at 3572 cm⁻¹, were detected 458 459 (Fig. 10). This confirms the mechanism of charge compensation with the creation of OH⁻ vacancies, and highlights the new environment and distribution of OH⁻ ions along the 460 channels of the SiHA structure [93, 97] and, more importantly, the formation of low hydrogen 461 bonding between closed O^{2-} and OH^{-} ions (H-bonds cause a shift of 20 cm⁻¹ to the low 462 wavenumber of the main band at 3572 cm⁻¹ [98]). The FT-IR spectrum of Si₁₀HA displays 463 the same eight new bands as those detected on Si_{0.25}HA, Si_{0.50}HA and Si_{0.75}HA. However, 464 their relative intensity decreased significantly, reaching the detection limit for the band at 750 465 cm^{-1} and with a complete disappearance of the bands at 491, 504, and 528 cm^{-1} . Additionally, 466 seven new vibrations appeared at 500, 515, 535, 683, 798 and 873 cm⁻¹. They were 467 accompanied by an intensification of the shoulder at 947 cm⁻¹. The bands at 683, 798 and 870 468 cm⁻¹ were also detected in spectrum of Si_{1.25}HA calcined powder. According to these results 469

and an accurate review of the bibliography, summarized in Table 4, it is clear that the nine 470 vibrations at 493, 504, 528, 750, 840, 893, 930, 985 and 1002 cm⁻¹ are related to the 471 incorporation of Si into the hydroxyapatite structure. The changes detected in the sample 472 Si₁₀HA were due to the start of decomposition of the SiHA phase, emphasized by a decrease 473 in the nine characteristic bands and the formation of an amorphous silica phase which 474 presents vibrations at 500, 515, 535, 683, 798 and 873 cm⁻¹. Silica was not detected by NMR 475 due to the low amount of ²⁹Si in the samples (high detection limit). The shoulder at 947 cm⁻¹ 476 could be attributed to β -TCP, which exhibits a symmetric P-O stretching mode v₁ at 945 cm⁻¹ 477 [96]. However, this assumption is not convincing since other bands assigned to β -TCP are 478 absent. In fact, this shoulder is a contribution of the Si-O in plane stretching vibrations in Si-479 OH and Si-O⁻ on the surface of the grains, and the symmetric stretching (v₁) vibration of 480 orthophosphate groups in the neighborhood of OH vacancies along the channels. The former, 481 reported at 950 cm⁻¹ (see Table 4), shifted toward lower frequencies due to hydrogen bonding 482 between surface groups, thus creating the component at 930 cm⁻¹. The band at 950 cm⁻¹ is 483 commonly observed for oxy-hydroxyapatite $Ca_{10}(PO_4)_6(OH)_{2-2x}O_x(V_{OH})_x$, [93, 99-102]. 484 Therefore, in the context of this study, OH⁻ vacancies (V_{OH}) are due first to the incorporation 485 of SiO₄ into the HA structure, and second to the partial dehydration of SiHA to SiOHA as 486 follows: 487

488
$$Ca_{10}(PO_4)_{6-v}(SiO_4)_{v}(OH)_{2-v}(V_{OH})_{v} \leftrightarrow Ca_{10}(PO_4)_{6-v}(SiO_4)_{v}(OH)_{2-v-2x}O_x(V_{OH})_{v+x} + x H_2O$$
 (7)

489 3.2.6.4. Calcined samples – OH vacancies and the limit of incorporation of Si in HA

The amount of hydroxide (%OH) in the silicon-substituted hydroxyapatite structure is reported versus the amount of silicon (mol mol_{SiHA}⁻¹) in Fig. 11. The theoretical values of OH were plotted by considering the formula $Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-y}(V_{OH})_y$ (*i.e.* %OH = 100 -50 y). The experimental values were determined at room temperature on the calcined samples (1000°C/15 h) by means of the integrated area of the v_L and v_S OH bands. The average of the

integrated areas obtained for HA (y=0) was assumed to be representative of the full 495 occupancy of the OH position within the channels (100% OH). The amount of OH vacancies 496 (V_{OH}) determined experimentally was always higher than the theoretical one with respect to 497 the chemical formula $Ca_{10}(PO_4)_{6-v}(SiO_4)_v(OH)_{2-v}(V_{OH})_v$. In other words, the dehydration of 498 the calcined powders was greater than expected, and a higher Si doping level led to a greater 499 difference. Thus, the incorporation of Si into the hydroxyapatite structure generates OH 500 vacancies first to maintain the charge balance $(Ca_{10}(PO_4)_{6-v}(SiO_4)_v(OH)_{2-v}(V_{OH})_v)$ and second 501 502 from another phenomena, which is an increasing function of the amount of Si. A possible explanation is an increase of the mobility of OH ions along the channel axis (local disorder) 503 and their subsequent rate of diffusion and debonding from the HA lattice [103]. HA 504 decomposition is a dynamic process, mainly controlled by the degree of dehydration [104-505 106]. In fact, the thermal stability of hydroxyapatite was found to depend on the fraction of 506 V_{OH} and O^{2-} ions in the channels. Several "critical values" of V_{OH} in OHA $Ca_{10}(PO_4)_6(OH)_{2-}$ 507 $_{2x}O_x(V_{OH})_x$ have been reported beyond which the apatite channel structure is destroyed: x \leq 508 509 0.80 [103], $x \le 0.75$ [107], $x \le 0.50$ [89]. However, the most probable limit comes from work 510 of Heughebaert and Montel on the crystallization of calcium phosphates during precipitation [108, 109]. They determined that the apatitic structure appears only when at least 25% of the 511 OH⁻ positions along the channels are really occupied. In other words, the apatitic structure 512 appears when $V_{OH} < 1.5$. Therefore, the theoretical maximum limit of incorporation of Si into 513 a hexagonal apatitic structure is y < 1.5 as regards the formula $Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y}(OH)_{1-y$ 514 $_{\rm v}(V_{\rm OH})_{\rm v}$. However, due to the dehydration reaction (Eq. 7), this limit is a function of the 515 516 temperature and the atmosphere of heat treatment. This assumption can explain why the Si₁₀HA and Si₁₂₅HA powders, which showed an apatitic structure after calcination at 400°C 517 518 for 2 h, were not thermically stable at 1000°C for 15 h in contrast to SiHA with a silicon content ranging between $0 \le y \le 0.75$. Control of the degree of hydroxylation, *i.e.* the partial 519

steam pressure p_{H20} , is necessary to control the thermal stability of the SiHA phase. This 520 assumption is confirmed by the infrared spectra obtained from the Si_{1.0}HA sample heat treated 521 at 1000°C for 15 h under different partial pressures of steam, p_{H20}, in mbar (Fig. 12); a higher 522 p_{H20} led to a more stable silicon-substituted apatite phase. Thus, the Si₁₀HA powder, after 523 calcination under high steam pressure ($p_{H20} = 200$ mbar), presented only the characteristic 524 bands of SiHA with traces of amorphous silica at the IR spectroscopy detection limit 525 (≈ 0.1 wt%), whereas the same sample heat-treated under dry argon gas (pH₂O = 0 mbar) 526 contained amorphous silica species as well as TCP (α and β). Moreover, the vibrations related 527 to Si-O in SiHA (750 and 890 cm⁻¹) as well as the vibrational modes v_3 and v_4 of the phosphate 528 groups in HA decreased with a decrease in p_{H20} . Conversely, the vibrations due to amorphous 529 silica species, at 683, 798 and 873 cm⁻¹, and TCP (e.g. 731, 942, 997 and 1137 cm⁻¹) increases 530 with a decrease in p_{H20} . 531

These results confirm that the formation of amorphous silica and the decomposition of the SiHA phase are correlated. More precisely, the detection of amorphous silica indicates the start of decomposition, which is followed by the formation of TCP (α and β).

Finally, Trombe and Montel reported the variation of *a* from 9.421 Å to 9.402 Å, without a significant variation in the *c* lattice parameter, when HA transforms into OHA, $Ca_{10}(PO_4)_6(OH)_{0.5}O_{0.75}(V_{OH})_{0.75}$ [102]. Thus, SiHA dehydration can explain the random fluctuations in the *a* lattice parameter observed in this work and in the literature [30].

539 4. Conclusion

This paper presents a new route to synthesize monophasic silicon-containing hydroxyapatites $Ca_{10}(PO_4)_{6-y}(SiO_4)_y(OH)_{2-y}(V_{OH})_y$ (SiHAs) with controlled stoichiometry. The combination of solid state nuclear magnetic resonance (NMR) and IR spectroscopy (IR) demonstrated that silicate substitution for phosphate creates OH vacancies along the channels. Moreover, Si substitution increases the local disorder and the mobility of OH ions along these channels and

their subsequent rate of diffusion and debonding from the HA lattice. The control of the 545 degree of hydroxylation of the SiHA phases, *i.e.* their thermal stability, can be carried out by 546 means of the partial steam pressure, p_{H20}. Additionally, an exhaustive description of the 547 infrared bands related to the incorporation of silicate groups into the HA structure was 548 established. It allowed us to determine that the literature has incorrectly attributed some 549 infrared bands to silicate groups in the apatite structure. These bands, e.g. 683, 798 and 873 550 cm⁻¹, due in fact to amorphous silica phases, raise questions regarding the phase purity of the 551 552 great majority of biologically evaluated SiHA bioceramics.

- 553
- 554

555 Acknowledgments

The authors wish to thank the "Region Rhône-Alpes" for the financial support provided forthis work.

558

References

[1] Carlisle EM. Silicon: A Possible Factor in Bone Calcification. Science 1970;167:279-80.

[2] Carlisle EM. In vivo requirement for silicon in articular cartilage and connective tissue formation in the chick. The journal of nutrition 1976;106:478-84.

[3] Nielsen FH, Poellot R. Dietary silicon affect bone turnover differently in ovariectomized and sham-operated growing rats. The journal of the trace elements in experimental medecine 2004;17:137-49.

[4] Schwarz K, Milne D. Growth promoting effects of silicon in rats. Nature 1972;239 333-4.

[5] Damen JJM, M. TCJ. Silica-induced Precipitation of Calcium Phosphate in the Presence of Inhibitors of Hydroxyapatite Formation. Journal of dental Research 1992;71:453-7.

[6] Jugdaohsingh R. Silicon and bone health. The Journal of Nutrition Health and Aging 2007;11:99-110.

[7] Reffitt DM, Ogston N, Jugdaohsingh R, Cheung HFJ, Evans BAJ, Thompson RPH, et al. Orthosilicic acid stimulates collagen type 1 synthesis and osteoblastic differentiation in human osteoblast-like cells in vitro. Bone 2003;32:127-35.

[8] Gibson IR, Best SM, Bonfield W. Chemical characterization of silicon-substituted hydroxyapatite. J Biom Mat Res 1999;44:422-8.

[9] Patel N, Best SM, Bonfield W, Gibson IR, Hing KA, Damien E, et al. A comparative study on the in vivo behavior of hydroxyapatite and silicon substituted hydroxyapatite granules. J MatSci: Materials in Medicine 2002;13:1199-206.

[10] Arcos D, Rodríguez-Carvajal J, Vallet-Regí M. The effect of the silicon incorporation on the hydroxylapatite structure. A neutron diffraction study. Solid State Sciences 2004;6:987-94.

[11] Astala R, Calderin L, Yin X, Stott MJ. Ab Initio Simulation of Si-Doped Hydroxyapatite. Chem Mat 2006;18:413-22.

[12] Gibson IR, Huang J, Best SM, Bonfield W. Enhanced *in vitro* cell activity and surface apatite layer formation on novel silicon-substituted hydroxyapatites. Bioceramics 1999;12:191-4.

[13] Best S, Bonfield W, R. Gi, Jha LJ, Da Silva Santos JD. Silicon-substituted apatites and process for the preparation thereof. United States Patent, US 6,312,468 B1

Great Britain, London1998.

[14] Thian ES, Huang J, Vickers ME, Best SM, Barber ZH, Bonfield W. Silicon-substituted hydroxyapatite (SiHA): A novel calcium phosphate coating for biomedical applications. Journal of Materials science 2006;41:709-17.

[15] Vallet-Regí M, Arcos D. Silicon substituted hydroxyapatites. A method to upgrade calcium phosphate based implants. Journal of Materials chemistry 2005;15.

[16] Gasquères G, Bonhomme C, Maquet J, Babonneau F, Hayakawa S, Kanaya T, et al. Revisiting silicate substituted hydroxyapatite by solid-state NMR. Magn Reson Chem 2008;46:342-6.

[17] Tang XL, Xiao XF, Liu RF. Structural characterization of silicon-substituted hydroxyapatite synthesized by a hydrothermal method. Materials Letters 2005;59:3841-6.

[18] Gomes S, Nedelec J-M, Jallot E, Sheptyakov D, Renaudin G. Silicon location in silicatesubstituted caclium phosphate ceramics determined by neutron diffraction. Crystal growth and design 2011;11:4017-26.

[19] Kim SR, Lee JH, Kim YT, Riu DH, Jung SJ, Lee YJ, et al. Synthesis of Si, Mg substituted hydroxyapatites and their sintering behaviors. Biomaterials 2003;24:1389-98.

[20] Ruys AJ. Silicon-doped hydroxyapatite. Journal of the Australian ceramic society 1993;29:71-80.

[21] Putlayev V, Veresov A, Pulkin M, Soin A, Kuznetsov V. Silicon-substituted hydroxyapatite ceramics (Si-HAP): densification and grain growth through the prism of sintering theories. Materials Science and Engineering Technology 2006;37:416-21.

[22] Best SM, Zou S, Brooks RA, Huang J, Rushton N, Bonfield W. The osteogenic behaviour of silicon substituted hydroxyapatite. Key Engineering Materials 2008;361-363:985-8.

[23] Hing KA, Revell PA, Smith N, Buckland T. Effect of silicon level on rate, quality and progression of bone healing within silicate-substituted porous hydroxyapatite scaffolds. Biomaterials 2006;27:5014-26.

[24] Bothelo CM, Brooks RA, Best SM, Lopes MA, Santos JD, Rushton N, et al. Human osteoblast response to silicon-substituted hydroxyapatite. Journal of Biomedical Materials Research 2006;79A:723-30.

[25] Thian ES, Huang J, Best SM, Barber ZH, Brooks RA, Rushton N, et al. The response of osteoblasts to nanocrystalline silicon-substituted hydroxyapatite thin films. Biomaterials 2006;27:2692-8.

[26] Hing KA, Wilson LF, Buckland T. Comparative performance of three ceramic bone graft substitutes. The Spine Journal 2007;7:475-90.

[27] Palard M, Combes J, Champion E, Foucaud S, Rattner A, Bernache-Assollant D. Effect of silicon content on the sintering and biological behaviour of $Ca_{10}(PO_4)_{6-x}(SiO_4)_x(OH)_{2-x}$ ceramics. Acta Biomaterialia 2009;5:1223-32.

[28] Boanini E, Gazzano M, Bigi A. Ionic substitutions in calcium phosphates synthesized at low temperature. Acta Biomaterialia 2010;6:1882-94.

[29] Bohner M. Silicon-substituted calcium phosphates – A critical view. Biomaterials 2009;30:6403-6.

[30] Gomes S, Renaudin G, Mesbah A, Jallot E, Bonhomme C, Babonneau F, et al. Thorough analysis of silicon substitution in biphasic calcium phosphate bioceramics: A multi-technique study. Acta Biomaterialia 2010;6:3264-74.

[31] Langstaff S, Sayer M, Smith TJN, Pugh SM. Resorbable bioceramics based on stabilized calcium phosphates. Part II: evaluation of biological response. Biomaterials 2001;22:135-50.

[32] Palard M, Champion E, Foucaud S. Synthesis of silicated hydroxyapatite $Ca_{10}(PO_4)_{6-x}(SiO_4)_x(OH)_{2-x}$. Journal of Solid State Chemistry 2008;181:1950-60.

[33] Pietak AM, Reid JW, Sayer M. Electron spin resonance in silicon substituted apatite and tricalcium phosphate. Biomaterials 2005;26:3819-30.

[34] Reid JW, Tuck L, Sayer M, Fargo K, Hendry JA. Synthesis and characterization of single-phase silicon-substituted α -tricalcium phosphate. Biomaterials 2006;27:2916-25.

[35] Tang Q, Brooks RA, Rushton N. Production and characterization of HA and SiHA coatings. Journal of Materials Science: Materials in Medicine 2010;21:173-81.

[36] Arcos D, Rodríguez-Carvajal J, Vallet-Regí M. Silicon incorporation in hydroxyapatite obtained by controlled crystallization. Chemistry of materials 2004;16:2300-8.

[37] Balas F, Pérez-Pariente J, Vallet-Regí M. *In vitro* bioactivity of silicon-substituted hydroxyapatites. Journal of Biomedical Materials Research Part A 2003;66A:364-75.

[38] Kanaya T, Tsuru K, Hayakawa S, Osaka A, Fujii E, Kowabata K, et al. Structure and *in vitro* solubility of silicon-substituted hydroxyapatite. Key Engineering Materials 2008;361-363:63-6.

[39] Botelho CM, Lopes MA, Gibson IR, Best SM, Santos JD. Structural analysis of Sisubstituted hydroxyapatite: zeta potential and X-ray photoelectroscopy. J Mat Sc 2002;13:1123-7.

[40] Bothelo CM, Brooks RA, Best SM, Lopes MA, Santos JD, Rushton N, et al. Biological and physical-chemical characterization of phase pure HA and Si-Substituted Hydroxyapatite by different microscopy techniques. Key Engineering Materials 2004;254-256:845-8.

[41] Bothelo CM, Brooks RA, Kawai T, Ogata S, Ohtsuki C, Best SM, et al. *In vitro* analysis of protein adhesion to phase pure hydroxyapatite and silicon substituted hydroxyapatite. Key Engineering Materials 2005;284-286:461-4.

[42] Bothelo CM, Brooks RA, Spence G, I. M, Lopes MA, Best SM, et al. Differenciation of mononuclear precursors into osteoclasts on the surface of Si-Substituted hydroxyapatite. Journal of biomedical Materials research part A 2006;78A:709-20.

[43] Bothelo CM, Stokes DJ, Brooks RA, Best SM, Lopes MA, Santos JD, et al. Effect of the human serum proteins on pure hydroxyapatite and silicon substituted hydroxyapatite: AFM and SEM studies. Materials Science Forum 2004;455-456:378-82.

[44] Gibson IR, Best SM, Bonfield W. Effect of Silicon substitution on the sintering and microstructure of hydroxyapatite. Journal of the American Ceramic Society 2002;85:2771-7.

[45] Gupta G, Kirakodu S, El-Ghannam A. Dissolution kinetics of a Si-rich nanocomposite and its effect on osteoblast gene expression. Journal of Biomedical Materials Research 2006;80A:486-96.

[46] Guth K, Campion C, Buckland T, Hing KA. Effect of Silicate-Substitution on Attachment and Early Development of Human Osteoblast-Like Cells Seeded on Microporous Hydroxyapatite Discs. Advanced Engineering Materials 2010;12:1527-2648.

[47] Guth K, Campion C, Buckland T, Hing KA. Effects of serum protein on ionic exchange between culture medium and microporous hydroxyapatite and silicate-substituted hydroxyapatite. Journal of Materials Science: Materials in Medicine 2011;22:2155-64.

[48] Hijón N, Victoria Cabañas M, Peña J, Vallet-Regí M. Dip coated silicon-substituted hydroxyapatite films. Acta Biomaterialia 2006;2:567-74.

[49] Lehmann G, Palmero P, Cacciotti I, Pecci R, Campagnolo L, Bedini R, et al. Design production and biocompatibility of nanostructured porous HAp and SiHAp ceramics as three dimensional scaffolds for stem cell culture and. Ceramics – Silikáty 2010;54:90-6.

[50] Leventouri T, Bunaciu CE, Perdikatsis V. Neutron powder diffraction studies of siliconsubstituted hydroxyapatite. Biomaterials 2003;24:4205-11. [51] López-Álvarez M, Solla EL, González P, Serra J, León B, Marques AP, et al. Siliconhydroxyapatite bioactive coatings (Si–HA) from diatomaceous earth and silica. Study of adhesion and proliferation of osteoblast-like cells. Journal of Materials Science: Materials in Medicine 2009;20:1131-6.

[52] Martinez IM, Velasquez PN, De Aza PN. Synthesisans stability of a-tricalcium phosphate doped with dicalcium silicate in the system $Ca_3(PO_4)_2$ - Ca_2SiO_4 . Materials Characterization 2010;61:761-7.

[53] Porter AE, Patel N, Skepper JN, Best SM, Bonfield W. Comparison of in vivo dissolution processes in hydroxyapatite and silicon-substituted hydroxyapatite bioceramics. Biomaterials 2003;24:4609-20.

[54] Seet SL. Silicon-substituted calcium phosphate compounds - Synthesis characterizationa nd biological evaluation (Fumed silica). Science Asia 2009;35:255-60.

[55] Marques da Silva H, Mateescu M, Ponche A, Damia C, Champion E, Soares G, et al. Surface transformation of silicon-doped hydroxyapatite immersed in culture medium under dynamic and static conditions. Colloids and Surfaces B: Biointerfaces 2010;75:349-55.

[56] Sprio S, Tampieri A, Landi E, Sandri M, Martorana S, Celotti G, et al. Physico-chemical properties and solubility behaviour of multi-substituted hydroxyapatite powders containing silicon. Materials Science and Engineering: C 2008;28:179-87.

[57] Vandiver J, Dean D, Patel N, Botelho C, Best SM, Santos JD, et al. Silicon addition to hydroxyapatite increases nanoscale electrostatic, van der Waals, and adhesive interactions. Journal of Biomedical Materials Research Part A 2006;78A:352-63.

[58] Zou S, Ireland D, Brooks RA, Rushton N, Best S. The effects of silicate ions on human osteoblast adhesion, proliferation, and differentiation. Journal of Biomedical Materials Research Part B: Applied Biomaterials 2009;90B:123-30.

[59] Arcos D, Sanchez-Salcedo S, Izquierdo-Barba I, Ruiz L, Gonzalez-Calbet J, Vallet-Regí M. Crystallochemistry, textural properties, and *in vitro* biocompatibility of different silicondoped calcim phosphates. Journal of Biomedical Materials Research 2006;78A:762-71.

[60] Bakunova N, Fomin A, Fadeeva I, Barinov S, Shvorneva L. Silicon-containing hydroxylapatite nanopowders. Russian Journal of Inorganic Chemistry 2007;52:1492-7.

[61] Thian ES, Huang J, Best SM, Barber ZH, Bonfield W. Silicon-substituted hydroxyapatite: The next generation of bioactive coatings. Symposium A: Advanced Biomaterials International Conference on Materials for Advanced Technologies (ICMAT 2005) 2007;27:251-6.

[62] Huang T, Xiao Y, Wang S, Huang Y, Liu X, Wu F, et al. Nanostructured Si Mg CO₃ Hydroxyapatite Coatings Deposited by Liquid Precursor Plasma Spraying. Journal of the thermal spray technology 2011;20:829-36.

[63] Gillespie P, Wu G, Sayer M, Stott MJ. Si complexes in calcium phosphate biomaterials. Journal of Materials Science: Materials in Medicine 2010;21:99-108.

[64] Langstaff S, Sayer M, Smith TJN, Pugh SM, Hesp SAM, Thompson WT. Resorbable bioceramics based on stabilized calcium phosphates. Part I: rational design, sample preparation and material characterization. Biomaterials 1999;20:1727-41.

[65] Reid JW, Pietak A, Sayer M, Dunfield D, Smith TJN. Phase formation and evolution in the silicon substituted tricalcium phosphate/apatite system. Biomaterials 2005;26:2887-97.

[66] Sayer M, Stratilatov AD, Reid J, Calderin L, Stott MJ, Yin X, et al. Structure and composition of silicon-stabilized tricalcium phosphate. Biomaterials 2003;24:369-82.

[67] Borsa R-N. Elaboration de poudres et de dépôts de phosphates de caclium silicatés à usage de biomatériaux. Toulouse: Université de Toulouse; 2008.

[68] Aminian A, Solati-Hashjin M, Samadikuchaksaraei A, Bakhshi F, Gorjipour F, Farzadi A, et al. Synthesis of silicon-substituted hydroxyapatite by a hydrothermal method with two different phosphorous sources. Ceramics International 2011;37:1219-29.

[69] Kim YH, Song H, Riu DH, Kim SR, Kim HJ, Moon JH. Preparation of porous Siincorporated hydroxyapatite. Current Applied Physics 2005;5:538-41.

[70] Tian T, Jiang D, Zhang J, Lin Q. Synthesis of Si-substituted hydroxyapatite by a wet mechanochemical method. Materials Science and Engineering: C 2008;28:57-63.

[71] Solla EL, Gonzalez P, Serra J, Chuiussi S, Leon B, Garcia Lopez J. Pulsed laser deposition of silicon substituted hydroxyapatite coatings from synthetical and biological sources. Applied Surface Science 2007;254:1189-93.

[72] Xiao XF, Liu RF, Tang XL. Electrophoretic deposition of silicon substituted hydroxyapatite coatings from n-butanol-chloroform mixture. Journal of Materials Science: Materials in Medicine 2008;19:175-82.

[73] Panteix P-J, Bécahde E, Julien I, Abélard P, Bernache-Assollant D. Influence of anionic vacancies on the ionic conductivity of silicated rare earth apatites. Materials Research Bulletin 2008;43:1223-31.

[74] Bianco A, Cacciotti I, Lombardi M, Montanaro L. Si-substituted hydroxyapatite nanopowders: Synthesis, thermal stability and sinterability. Materials Research Bulletin 2009;44:345-54.

[75] Porter AE, Patel N, Skepper JN, Best SM, Bonfield W. Effect of sintered silicatesubstituted hydroxyapatite on remodelling processes at the bone–implant interface. Biomaterials 2004;25:3303-14.

[76] Marques PAAP, Magalhaes MCF, Correia RN, Vallet-Regí M. Synthesis and characterization of silicon-substituted hydroxyapatite. Key Engineering Materials 2001;192-195:247-50.

[77] Plokhikh NV, Soin AV, Kuztnetsov AV, Veresov AG, Putlayev VI, Tretyakov YD. Synthesis of silico-substituted hydroxyapatite. Mendeleev Communications 2004;14:178-9.

[78] Mostafa NY, Hassan HM, Abd Elbader OH. Preparation and Characterization of Na⁺, $SiO_4^{4^+}$, and $CO_3^{2^-}$, Co-Substituted Hydroxyapatite. Journal of the American Ceramic Society 2011;94:1584-90.

[79] Mostafa NY, Hassan HM, Mohamed FH, Omar H. Preparation of Na^+ , SiO_4^{4-} and CO_3^{2-} co-substituted hydroxyapatite nanoparticles. Materials Research Bulletin 2009;In Press, Accepted Manuscript.

[80] Klein LC, Woodman RH. Porous silica by the Sol-Gel Process. Key Engineering Materials 1996;115:109-24.

[81] Elliott JC. Structure and Chemistry of the Apatites and Other Calcium Orthophosphates. Amsterdam-London-New York-Tokyo: Elsevier; 1994.

[82] Sefcik J, McCormick V. Thermochemistry of aqueous silicate solution precursors to ceramics. Ceramics Processing 1997;43:2773-84.

[83] Lafon JP, Champion E, Bernache-Assollant D. Processing of AB-type carbonated hydroxyapatite Ca10-x(PO4)6-x(CO3)x(OH)2-x-2y(CO3)y ceramics with controlled composition. Journal of the European Ceramic Society 2008;28:139-47.

[84] Rey C, Collins B, Goehl T, Dickson IR, Glimcher MJ. The carbonate environment in bone mineral: a resolution enhanced Fourier transform infrared spectroscopy study. Calcified Tissue International 1989;45:157-64.

[85] Mostafa NY, Hassan HM, Mohamed FH. Sintering behavior and thermal stability of Na⁺, SiO_4^{4-} and CO_3^{2-} co-substituted hydroxyapatites. Journal of Alloys and Compounds 2009;479:692-8.

[86] Marchat D, Bernache-Assollant D, Champion E. Cadmium fixation by synthetic hydroxyapatite in aqueous solution - Thermal behaviour. First International Conference on Engineering for Waste Treatment: Beneficial Use of Waste and By-Products (WasteEng2005) 2007;139:453-60.

[87] Stadelmann P. Java Electron Microscopy Simulation (JEMS) software. Switzerland: CIME-EPFL, École Polytechnique Fédérale de Lausanne; 1999-2006.

[88] Miquel JL, Facchini L, Legrand AP, Marchandise X, Lecouffe P, Chanavaz M, et al. Characterization of bioacceptable carbon materials. Clinical Materials 1990;5:115-25.

[89] Hartmann P, Barth S, Vogel J, Meyer K. Solid State NMR, X-Ray Diffraction, and Infrared Characterization of Local Structure in Heat-Treated Oxyhydroxyapatite Microcrystals: An Analog of the Thermal Decomposition of Hydroxyapatite during Plasma-Spray Procedure Journal of Solid State Chemistry 2001;160:460-8.

[90] Bonhomme C, Babonneau F, Azaïs T, Coelho C, Aimé C, Quignard S, et al. Dynamic Nuclear Polarization (DNP) for the characterization of nanoparticles. The Journal of Physical Chemistry 2012;(Submitted).

[91] Arends J, Christoffersen J, Christoffersen MR, Eckert H, Fowler BO, Heughebaert JC, et al. A calcium hydroxyapatite precipitated from an qaueous solution. Journal of Crystal Growth 1987;84.

[92] Rey C, Shimizu M, Collins B, Melvin JG. Resolution-enhanced Fourier transform infrared spectroscopy study of the environment of phosphate ions in the early deposits of a solid phase of calcium-phosphate in bone and enamel, and their evolution with age. 1: Investigations in the n_4 PO₄ Domain. Calcified Tissue International 1990;46:384-94.

[93] Park E, Condrate SRA, Lee D, Kociba K, Gallagher PK. Characterization of hydroxyapatite: before and after plasma spraying. Journal of Materials Science 2002;13:211-8.

[94] Rey C, Shimizu M, Collins B, Glimcher J. Resolution-enhanced Fourier transform infrared spectroscopy study of the environment of phosphate ions in the early deposits of a solid phase of calcium-phosphate in bone and enamel, and their evolution with age. 2: Investigations in the $n_3 PO_4$ Domain. Calcified Tissue International 1991;49:383-8.

[95] Zymelka M, Marchat D, Szenknect S, Dacheux N, Bernache-Assollant D, Chevalier J. Silicon-substituted hydroxyapatite particles precipitation and dissolution. Acta Biomaterialia 2012;(Submitted).

[96] Jillavenkatesa A, Condrate RA. The infrared and Raman spectra of b and a tricalcium phosphate $(Ca_3(PO_4)_2)$. Spectroscopy letters 1998;31:1619-34.

[97] Sänger AT, F. K. Structural disorder in hydroxyapatite. Zeitschrift für Kristallographie 1992;199:123-48.

[98] Hamilton WC, Ibers JA. Hydrogen Bonding in Solids. WA Benjamin : New-York 1968:204-21.

[99] Liao C-J, Lin F-H, Chen K-S, Sun J-S. Thermal decomposition and reconstitution of hydroxyapatite in air atmosphere. Biomaterials 1999;20:1807-13.

[100] Radin SR, Duchyene P. Plasma spraying induced changes of calcium phosphate ceramic characteristics and the effect on *in vitro* stability. Journal of Materials Science: Materials in Medicine 1992;3:33-42.

[101] Trombe J-C. Mise en évidence d'oxygène à différents degrés d'oxydation dans le réseau des apatites phosphocalciques et phosphostrontiques,. Annales de Chime 1973;8:335-47.

[102] Trombe J-C, Montel G. Some features of the incorportaion of oxygen in different oxidation states in the apatitic lattice - II on the synthesis and properties of calcium and strontium peroxiapatites

Journal of Inorganic and Nuclear Chemistry 1978;40:23-6.

[103] Wang T, Dorner-Reisel A, Müller E. Thermogravimetric and thermokinetic invetsigation of the dehydroxylation of hydroxyapatite powder. Journal of the European Ceramic Society 2004;24:693-8.

[104] Bernache-Assollant D, Ababou A, Champion E, Heughebaert M. Sintering of calcium phosphate hydroxyapatite $Ca_{10}(PO_4)_6(OH)_2$, I. Calcination and particle growth. Journal of the European Ceramic Society 2003;23:229-41.

[105] Liu Y, Shen Z. Dehydroxyalation of hydroxyapatite in dense bulk ceramics sintered by spark plasma sintering. ECERS 2012;32:2691-6.

[106] Trombe J-C, Montel G. Some features of the incorporation of oxygen in different oxidation states in the apatitic lattice - I. On the existence of calcium and strontium oxyapatite. Journal of Inorganic and Nuclear Chemistry 1978;40:15-21.

[107] Seuter AMJH. Existence Region of Calcium Hydroxyapatite and the

Equilibrium with Coexisting Phases at Elevated Temperatures. In: Anderson J.S RMW, Stone F.S., editor. Reactivity

of Solids1972.

[108] Heughebaert JC. Contribution à l'étude de l'évolution des orthophosphates de calcium précipités amorphes en orthophosphates apatitiques [Sciences physiques]. Toulouse: Institut National Polytechnique; 1977.

[109] Heughebaert JC, Montel G. Étude de l'évolution de l'orthophosphate tricalcique non cristallin en phosphate apatitique à la faveur d'une réaction chimique à température ordinaire. Revue de Physique Appliquée 1977;12:691-4.

[110] Aguiar H, Serra J, González P, León B. Structural study of sol–gel silicate glasses by IR and Raman spectroscopies. Journal of Non-Crystalline Solids 2009;355:475-80.

[111] Guerrero A, Goni S, A. M, Dolado JS. Microstructure and mechanical performance of Belite cements from high calcium coal fly ash. Journal of American Ceramic Society 2005;88:1845-53.

[112] Hollenstein C, Howling AA, Courteille C, Magni D, M. SS, Kroesen GMW, et al. Silicon oxide particle formation in RF plasmas investigated by infrared absorption spectroscopy and mass spectrometry. Journal of Physics D: Applied Physics 1998;31:74-84.

[113] Dunfield D, Sayer M, Shurvell HF. Total Attenuated Reflection Infrared Analysis of Silicon-Stabilized Tri-Calcium Phosphate. The Journal of Physical Chemistry B 2005;109:1957919583-19583.

[114] Al-Oweini R, El-Rassy H. Synthesis and characterization by FTIR spectroscopy of silica aerogels prepared using several Si(OR)4 and R"Si(OR')3 precursors. Journal of Molecular Structure 2009;919:140-5.

[115] Fidalgo A, Ilharco LM. The defect structure of sol-gel derived silica/polytetrahydrofuran hybrid films by FTIR. Journal of Non-Crystalline Solids 2001;283:144-54.

[116] Gopal NO, Narasimhulu KV, Rao JL. EPR, optical, infrared and Raman spectral studies of Actinolite mineral. Spectrochimica Acta 2004;60:2441-8.

[117] Alekhina LG, Akhmanova MV, Dement'ev VA, Gribov LA. Solution of the inverse spectroscopic problem for the SiO4 group. Journal of Applied Spectroscopy 1975;22:546-9.

[118] Bensted J, Varma SP. Some applications of infrared and Raman spectroscopy in cement chemistry. Part 2 - Portland cement and its constituents. Cement Technology 1974;4:378-82.

[119] Dutta PK, Shieh D-C. Raman Spectarl Study of the composition of basic silicate solutions. Applied Spectroscopy 1985;39:343-6.

[120] Etchepare J. Interprétation des spectres de diffusion Raman de verres de silice binaires. Spectrochimica Acta 1970;26A:2147-54.

[121] Mollah MYA, Yu W, Schennach R, Cocke DL. A fourier transform infrared spectroscopic investigation of the early hydration of Portland cement and the influence of sodium lignosulfonate. Cement and concrete research 2000;30:267-73.

[122] Nakamura M, Mochizuki Y, usami K, Y. I, T. N. Infrared absorption spectra and compositions of evaporated silicon oxides (SiO_x) . Solid State Communications 1984;50:1079-81.

[123] Theil JA, Tsu DV, Watkins MW, Kim SS, Lucovsky G. Local bonding environment of Si-OH groups in SiO_2 deposited by remote plasma-enhanced chemical vapor deposition and incorporated by postdeposition exposure to water vapor. American Vacuum Society 1990;A8:1374-81.

[124] Socrates G. Infrared and Raman characteristic group frequencies : Tables and Charts2004.

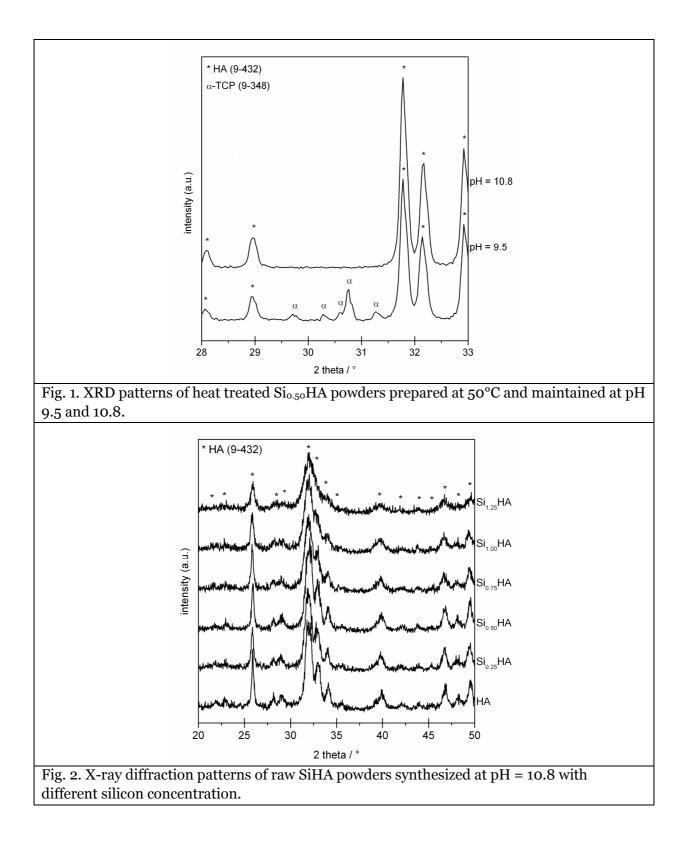
[125] Bell RJ, Bird NF, Dean P. The vibrational spectra of vitreous silica, germania and beryllium fluoride Journal of Physics C: Solid State Physics 1968;1:299-303.

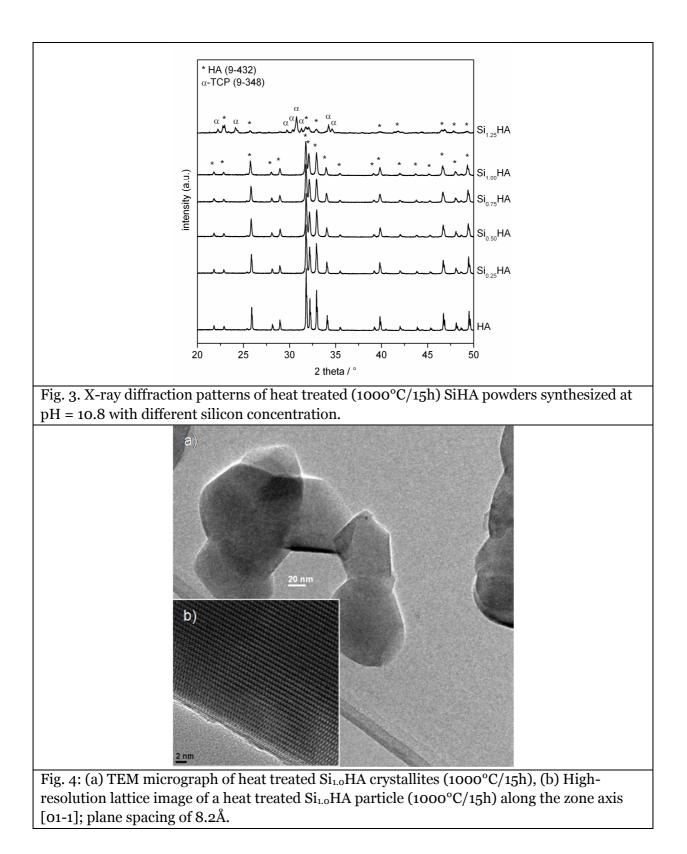
[126] Sato RK, McMillan PF. An infrared and Raman study of the isotopic species of alphaquartz. The Journal of Physical Chemistry B 1987;91:3494-8. [127] Sitarz M, Handke M, Mozgawa W. Identification of silicooxygen rings in SiO₂ based on IR spectra. Spectrochimica Acta Part A: Molecular and Biomolecular Spectroscopy 2000;56:1819-23.

[128] Ahsan MR, Mortuza MG. Infrared spectra of xCaO(1-x-z)SiO₂ zP₂O₅ glasses. Journal of Non-Crystalline Solids 2005;351:2333-40.

[129] Bosomworth DR, Hayes W, Spray ARL, Watkins GD. Absorption of Oxygen in Silicon in the Near and the Far Infrared Proceedings of the Royal Society (London) 1970;317:133-52.

[130] Sari SO, Hollingsworth-Smith P, Oona H. Near IR absorption in films of silicon containing oxygen. Journal of Physics and Chemistry of Solids 1978;39:857.





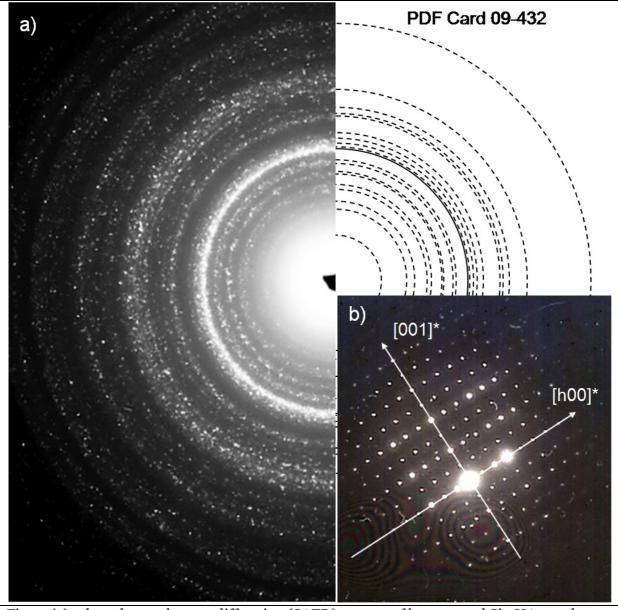
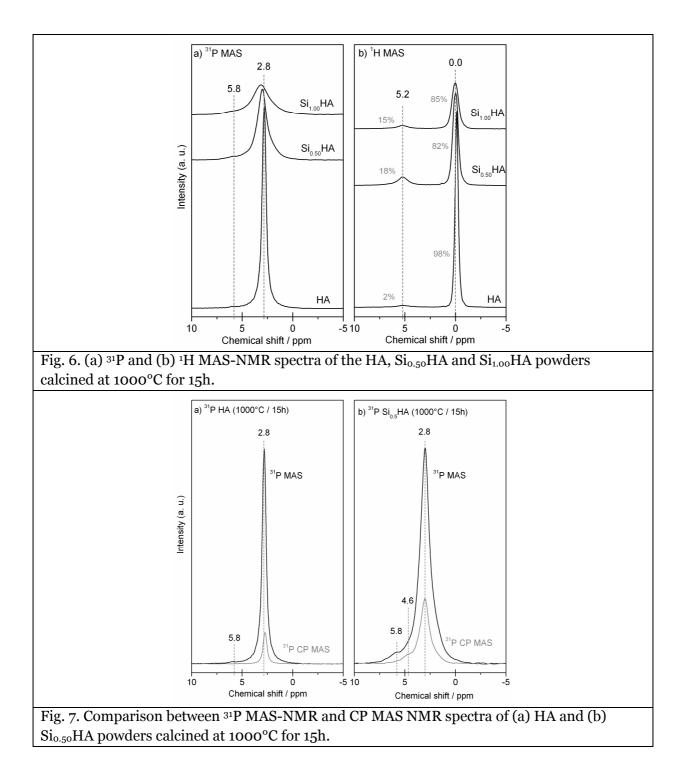
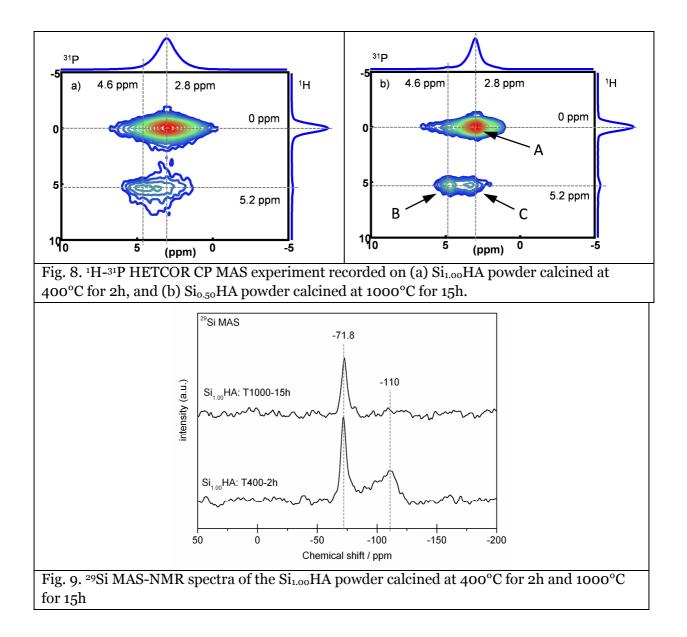
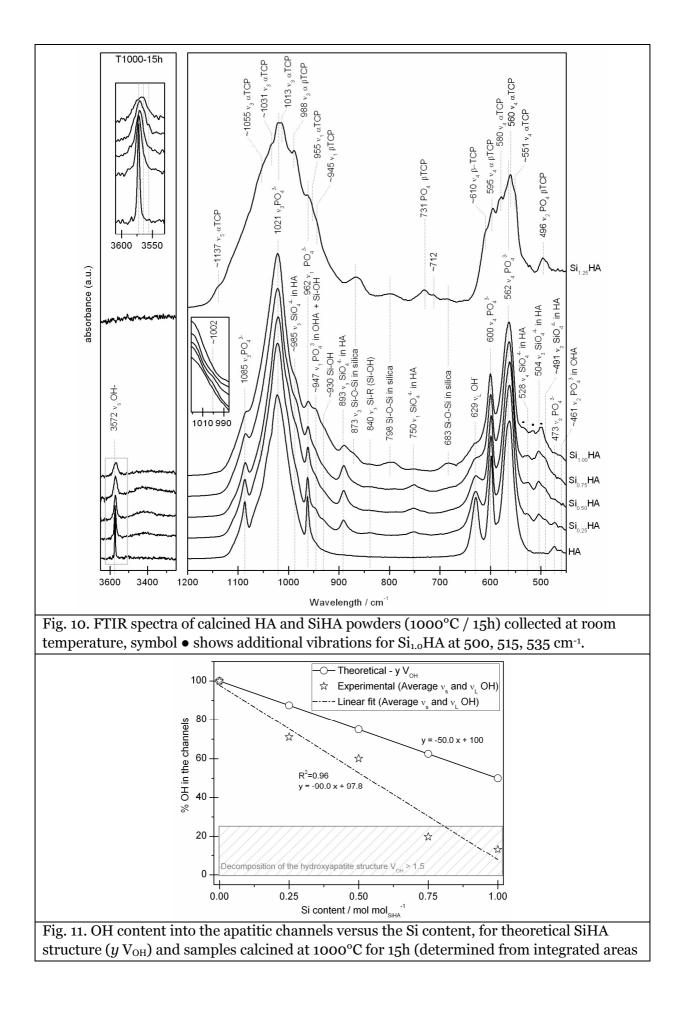


Fig. 5: (a) selected area electron diffraction (SAED) pattern of heat treated Si_{1.0}HA powder (1000°C/15h), (b) SAED of heat treated Si_{1.0}HA powder (1000°C/15h) for the [0 1 0] zone axis, c/a = 0.730







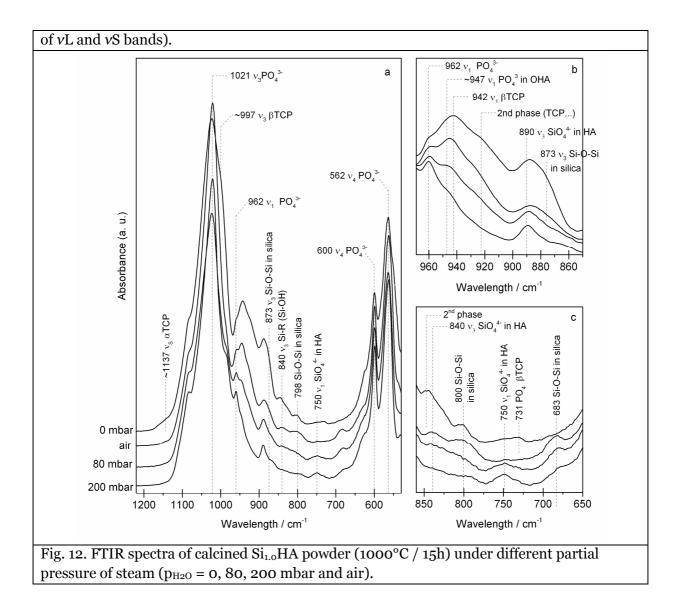


Table 1

Chemical conditions of preparation of HA and SiyHA samples and final composition of the

	Synthesis parameters $(T = 50^{\circ}C, t_m = 24h)$					Composition of the final calcined powders (1000°C/15h)			
G 1	n _{Ca}	n _P	n _{Si}	pН	ysi	ysi	Chemical formula of SiyHA	Ca/(P+Si)	
Sample					Expected	Determined - According to Equation Eq. 2		Determined by	
	/ mol	/ mol	/ mol	-	/ mol m	ol ⁻¹ _{SiHA}	-	ICP/AES	
HA	0.200	0.120	0	9.5	0	0	Ca10(PO4)6(OH)2	1.69 ± 0.05	
Si _{0.25} HA	0.200	0.115	0.005	11.0	0.25	0.28±0.02	$Ca_{10}(PO_4)_{5.72}(SiO_4)_{0.28}(OH)_{1.72}(V_{OH})_{0.28}$	1.69 ± 0.02	
Si _{0.50} HA	0.200	0.110	0.010	9.5	0.50	N/A	$HA + \alpha TCP$	N/A	
Si _{0.50} HA	0.200	0.110	0.010	11.0	0.50	0.52±0.02	$Ca_{10}(PO_4)_{5.48}(SiO_4)_{0.52}(OH)_{1.48}(V_{OH})_{0.52}$	1.68 ± 0.02	
Si _{0.75} HA	0.200	0.105	0.015	11.0	0.75	0.72±0.02	$Ca_{10}(PO_4)_{5.28}(SiO_4)_{0.72}(OH)_{1.28}(V_{OH})_{0.72}$	1.67 ±0.03	
Si _{1.00} HA	0.200	0.100	0.020	11.0	1.00	0.97±0.02	$Ca_{10}(PO_4)_{5.03}(SiO_4)_{0.97}(OH)_{1.03}(V_{OH})_{0.97}$	1.67 ± 0.01	
Si _{1.25} HA	0.200	0.095	0.025	11.0	1.25	N/A	HA+TCP	N/A	

calcined powders (1000°C/15h).

Table 2

NMR parameters.

NMR Experiments	t _{90°}	number of scans	relaxation delay	¹ H decoupling	contact time	t ₁ increments
	/ µs	-	/ s	-	/ ms	
¹ H MAS	4.6	4	300	-	-	-
³¹ P MAS	1.3	16	60		-	-
³¹ P CPMAS		16	15	SPINAL-64 (54kHz)	3	-
¹ H ⁻³¹ P HETCOR CPMAS	1.5	32			1	128
²⁹ Si MAS	1.5	~ 4000	60	SPINAL-64 (45kHz)	-	-

Table 3.

Lattice parameters, unit cell volume and mean size of the crystallites of heat-treated powders at 1000°C for 15h evaluated by Rietveld refinement.

Sampla	Lattice parameters /	Å	Volume of the unit cell / $Å^3$	Crystallites mean size / nm	
Sample	a-axis	c-axis	Volume of the unit cen / A		
PDF 9-432	9.418	6.884	1058	-	
HA	$9.421 \pm 3 \ 10^{-5}$	$6.884 \pm 3 \ 10^{-5}$	1058 ± 1	243 ± 1	
Si _{0,25} HA	$9.423 \pm 4 \ 10^{-5}$	$6.892 \pm 4 \ 10^{-5}$	1060 ± 1	157 ± 1	
Si _{0,50} HA	9.428 ± 2.10^{-4}	$6.899 \pm 2 \ 10^{-4}$	1062 ± 1	116±1	
Si _{0,75} HA	9.423 ± 2.10^{-4}	$6.908 \pm 2 \ 10^{-4}$	1062 ± 1	103 ± 1	
Si _{1,00} HA	$9.416 \pm 7 \ 10^{-5}$	$6.920 \pm 5 \ 10^{-5}$	1063 ± 1	107 ± 1	

Table 4

IR bands and	shoulders	assignment	proposed by o	ur work
in bands and	siloulueis	assignment	proposed by 0	ul wolk

λ / cm^{-1}	Mode assignments proposed by this work	Literature support
1002*	Degenerated PO_4^{3-} asymmetric stretching (v ₃)	[94, 110]
985	Si-OH at SiHA surface / and/or / Si in SiHA	[110-112]
947	Oxyapatite	[93, 99, 100, 102, 113]
947	Si-OH at SiHA surface	[114-116]
930**	Si-OH at SiHA surface / and/or / Si in SiHA	[114, 117-121]
893	Si in SiHA	[8, 113, 118]
873	Si in silica	[112, 113, 122, 123]
840	Si-R	[118, 124]
798	Si in silica	[34, 110, 112-115, 117, 120, 122, 125-127]
750	Si in SiHA	[32, 54, 74]
683	Si in silica	[113, 114, 116, 126, 127]
535	Si in silica	[128]
528	Si in SiHA	[111, 118, 121, 128]
515	Si in silica	[127-130]
504	Si in SiHA	[32, 56, 118]

* degeneration of the $v_3 PO_4^{3-}$ domain at 1020 cm⁻¹ due to the SiO₄⁴⁻ in the environment of the

phosphate ions

** degeneration of the band at 947 cm^{-1}