The effects of strontium-substituted bioactive glasses on osteoblasts and osteoclasts in vitro

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ABSTRACT

Bioactive glasses (BG) which contain strontium have the potential to combine the known bone regenerative properties of BG with the anabolic and anti-catabolic effects of strontium cations. Here we created a BG series (SiO2–P2O5–Na2O–CaO) in which 0–100% of the calcium was substituted by strontium and tested their effects on osteoblasts and osteoclasts in vitro. We show that ions released from strontium-substituted BG enhance metabolic activity in osteoblasts. They also inhibit osteoclast activity by both reducing tartrate resistant acid phosphatase activity and inhibiting resorption of calcium phosphate films in a dose-dependent manner. Additionally, osteoblasts cultured in contact with BG show increased proliferation and alkaline phosphatase activity with increasing strontium substitution, while osteoclasts adopt typical resorption morphologies. These results suggest that similarly to the osteoporosis drug strontium ranelate, strontium-substituted BG may promote an anabolic effect on osteoblasts and an anti-catabolic effect on osteoclasts. These effects, when combined with the advantages of BG such as controlled ion release and delivery versatility, may make strontium-substituted BG an effective biomaterial choice for a range of bone regeneration therapies.

1. Introduction

Osteoporosis is common among post-menopausal women and is marked by an imbalance in the normal process of bone remodelling. In osteoporotic bone, osteoclasts resorb too much bone while osteoblasts fail to create enough, which together disrupt the bone microarchitecture leaving it porous and prone to fracture. Annual direct costs due to osteoporosis-related fracture in the United States are estimated in the range of US$20 billion [1] and its disease burden in Europe is estimated to be greater than that attributed to any cancer save lung [2]. Strontium ranelate (SrR), sold under the trade name Protelos, is a drug approved for the treatment and prevention of osteoporosis and has been shown to reduce the number of hip and vertebral fractures in post-menopausal women [3,4]. The drug combines two atoms of stable strontium with the organic moiety ranelic acid. The cellular mode of action of SrR appears to be through the strontium cations themselves, which have been shown to work both in vivo and in vitro by stimulating osteoblasts to make new bone and preventing osteoclasts from resorbing bone [5,6]. That is, data suggest that SrR works by helping resident cells in the bone to restore the normal bone remodelling balance.

Bioactive glasses (BG) form a strong bond with living tissue via the formation of a hydroxyapatite layer on their surface [7] and have been used to repair hard tissues in a variety of craniofacial, maxillofacial, and periodontal applications [8]. BG particulate, for example, is used in a variety of dental procedures [9], and any BG compositions can be formed into scaffolds for tissue engineering [10]. Surface reactivity, however, is not their only mechanism of action as BG also release ions that promote the osteoblast phenotype [11,12]. In vitro studies have demonstrated that BG stimulate osteoprogenitors to differentiate to mature osteoblasts that produce bone-like nodules [13,14]. Similarly, in vivo studies have shown gradual degradation of implanted BG with subsequent formation of new bone at the implant surface [15,16]. Because of similarities in their charge and ionic radius, strontium can potentially be substituted for calcium in BG, creating a material that may combine the bone bonding and osteoblast stimulating properties of BG with the bone anabolic and anti-catabolic effects of strontium cations.
properties of SrR, and may act as an effective material for bone regeneration applications. Here we created a series of BG (SiO$_2$-P$_2$O$_5$-Na$_2$O-CaO) in which strontium was substituted for calcium on a mole percentage basis. We then tested their effects on cells cultured both in contact with the BG and treated with culture media containing ions released from the BG as they dissolved. The effects of strontium substitution in the BG were tested on osteoblast and osteoclast cultures and demonstrate that strontium-substituted BG promote osteoblast proliferation and activity and decrease osteoclast activity and resorption. As BG are a well-studied biomaterial and excellent system for controlled ion release, strontium-substituted BG may find use in a range of bone regeneration applications including as porous scaffolds, rigid materials and particulate.

2. Materials and methods

2.1. Bioactive glass synthesis

BG containing 46.46 SiO$_2$–1.07 P$_2$O$_5$–26.38 Na$_2$O–23.08 (SrO:CaO) (mole %) where neither calcium (0%) or 10, 50 or 100% of the calcium was substituted with strontium were produced by a melt-quench route as previously described [17]. Briefly, the composition was melted in a platinum crucible at 1400 °C for 90 min and rapidly quenched in deionised (dH$_2$O) water. BG frits were then ground and sieved to yield powders <38 μm in diameter. Some frits were then re-melted at 1450 °C and poured into pre-heated graphite moulds held just above the glass transition temperature (which varied between 450 and 500 °C depending on the percent strontium substitution [17]) to obtain rods 10 mm in diameter. Discs 1 mm thick were cut from the rods with a low speed diamond saw (Buehler IsoMet®Düsseldorf, Germany) using isopropanol as a coolant.

2.2. Dissolution ion studies

2.2.1. Dissolution ion media

1.5 g/L of BG powder was added to RPMI 1640 or Dulbecco’s modified Eagle’s (DMEM) cell culture medium (Invitrogen, Paisley, UK), incubated on a roller at 37 °C for 4 h and then passed over a 0.2 μm filter. Samples of dissolution ion media were collected after 10, 30, 60, 120, and 240 min for elemental analysis. Media were supplemented as described in Section 2.2.3 and equilibrated in a 37 °C/5% CO$_2$ incubator overnight before being placed on cells.

2.2.2. Elemental analysis

Cell culture media samples containing dissolution ions from BG were diluted by a factor of 10 in dH$_2$O and elemental concentrations of Ca, P and Sr ions were measured on an inductively coupled plasma – optical emission spectrometer (ICP-OES) (ICAP 6000, Thermo Scientific, Waltham, MA, USA).

2.2.3. Cell culture with dissolution ions

The human osteosarcoma cell line, Saos-2, was obtained from the European Collection of Cell Cultures (ECACC, Salisbury, UK) and routinely cultured under standard conditions (37 °C, 5% CO$_2$/95% air, 100% humidity) in RPMI 1640 media supplemented with 10% (v/v) foetal bovine serum (FBS) and 2 mM L-glutamine (all reagents from Invitrogen). For experiments, cells were plated at 30,000 cells/cm$^2$ and cultured for up to 28 days. The mouse monocyte cell line, RAW264.7, which differentiates to osteoclasts under appropriate conditions, was obtained from American Type Culture Collection (ATCC, Teddington, UK) and cultured in DMEM containing 4.5 g/L glucose and 1.5 g/L sodium bicarbonate (Sigma–Aldrich, Dorset, UK) supplemented with 10% (v/v) FBS and 4 mM L-glutamine. The nitrogenous bisphosphonate pamidronate (Sigma), a drug known to prevent osteoclast-mediated bone resorption in vivo [18], was added at a concentration of 1 μM as a control. For erosion pit studies, an additional control was created by adding 1 mM SrCl$_2$·6H$_2$O (Sigma) to standard cell culture medium. To initiate differentiation, 20 ng/mL soluble murine Receptor Activator for RANKL (Peprotech EC, London, UK) was added to the culture media of live cells at indicated time points. After 2 h, media was removed and the fomazan was solubilised in dimethyl sulfoxide. The absorbance of the resulting solution was read on a colorimetric plate reader at 592 nm.

2.2.4. Metabolic activity of cells

Cell metabolic activity was measured using the tetrazole MTT (3-(4,5-Dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide; Sigma), which is reduced to formazan by mitochondria in metabolically active cells. 50 μL of a 5 mg/mL solution of MTT in phosphate buffered saline (PBS) was added to the culture media of live cells at indicated time points. After 2 h, media was removed and the formazan was

2.2.5. Actin staining of cells

Differentiated RAW264.7 cultures were fixed for 15 min in 4% (w/v) paraformaldehyde in dH$_2$O. After fixation, cultures were washed in PBS, permeabilised in 1% (v/v) Triton X-100 in dH$_2$O for 5 min, washed again and then stained for 20 min with AlexaFluor 568 Phalloidin (Invitrogen; 5 μ/mL in 1% (v/v) bovine serum albumin (BSA) in PBS) to visualise the actin cytoskeleton. Cultures were then rinsed with 1% (v/v) BSA in PBS and DAPI was added to stain cell nuclei. Cultures were then imaged using an epifluorescent microscope.

2.2.6. Tartrate resistant acid phosphatase (TRAP) activity and total cell quantification

TRAP activity, a marker of osteoclast differentiation and resorbing activity [19], was measured in RAW264.7 cells by quantifying the conversion of p-nitrophenyl phosphate to p-nitrophenol in the presence of sodium tartrate under acidic conditions. After 2, 4, or 6 days in culture, cells were lysed in dH$_2$O by three freeze-thaw cycles and 1 mg/mL p-nitrophenyl phosphate in 0.1 μL glycine buffer with 0.1 mM ZnCl$_2$, 0.1 mM MgCl$_2$ and 20 mM sodium tartrate (pH 5.0) was added to the lysates. The reaction was stopped with 1 mL NaOH and the absorbance read at 405 nm on a colorimetric plate reader. TRAP activity is expressed as nmoles p-nitrophenol liberated per minute. The total number of cells in the same lysates was determined by quantifying the activity of the stable cytosolic enzyme lactate dehydrogenase with a CytoTox96® Non-Radioactive Cytotoxicity Assay (Promega, Southampton, UK), according to the manufacturer’s instructions.

2.2.7. Erosion pit formation by osteoclasts

The formation of erosion pits by differentiated RAW264.7 cells was evaluated using BioCoat™ Osteologic™ (BD Biosciences Europe, Erembodegem, Belgium) chamber well slides which were coated with a thin calcium phosphate (CaP) layer suitable for cell culture. 9600 cells/well were cultured for 4 days in the presence of 20 ng/mL RANKL with either no additional supplements, 1 mM SrCl$_2$·6H$_2$O, 1 μM pamidronate, or BG dissolution ion media. Cells were removed with sodium hypochlorite and slides stained with silver nitrate according to the manufacturer’s instructions. Micrographs of stained wells were taken on an inverted light microscope and the eroded area was determined using the histogram function in ImageJ (freeware from the NIH).

2.3. Bioactive glass discs studies

2.3.1. Cell culture on bioactive glass discs

BG discs were sterilised under UV light for 2 h per side and preconditioned for three days in RPMI 1640 medium (changed every day). 30,000 Saos-2 cells/cm$^2$ were seeded on BG discs and cultured for 1, 7, or 14 days in standard culture medium, which was exchanged three times per week. 50,000 RAW264.7 mouse monocytes/cm$^2$ were also seeded on 0% strontium-substituted BG discs and differentiated for 4 days in standard medium supplemented with 50 ng/mL RANKL to visualise osteoclast differentiation.

2.3.2. Scanning electron microscopy (SEM) of osteoclasts

After 4 days, RAW264.7 cells on 0% strontium-substituted BG discs were prepared for SEM imaging to view osteoclasts. Discs were washed twice in PBS and fixed in 2.5% (v/v) glutaraldehyde in 0.1% sodium cacodylate buffer (pH 7.3) for 40 min at 4 °C. Samples were then washed twice in PBS and dehydrated in a graded ethanol series followed by critical point drying with hexamethyldisilane. Following fixation, discs were sputter coated with gold and viewed on a Leo 1525 Gemini SEM operated at 10 kV.

2.3.3. Alkaline phosphatase (ALP) activity and total cell quantification

ALP activity, a marker of osteoblast differentiation and mineralisation, was measured in Saos-2 cultured on BG discs using the substrate p-nitrophenyl phosphate. At indicated time points, cultures were lysed in dH$_2$O containing 0.9% (v/v) Triton X-100 and reacted with 1 mg/mL p-nitrophenyl phosphate in 0.1 μL glycine buffer with 0.1 mM ZnCl$_2$ and 0.1 mM MgCl$_2$ (pH 10.4). The reaction was stopped with 1 mL NaOH and the absorbance read on a colorimetric plate reader at 405 nm. The total number of cells in the same lysates was determined using a CytoTox96® Non-Radioactive Cytotoxicity Assay according to the manufacturer’s instructions.

2.4. Statistical analyses

Statistical significance in MTT, TRAP and ALP assays was assessed by ANOVA with post-hoc LSD test to determine statistical significance between individual groups. A two-tailed Spearman’s ρ rank correlation was used to determine statistical significance in erosion pit area experiments. A ρ value of less than 0.05 was considered statistically significant. For experiments on BG discs, n = 6 per composition point per time point. Erosion pit area data represent means of 2 experiments and average data from at least 4 wells.
3. Results

3.1. Bioactive glass formation

BG frits and rods were optically clear and were shown to be amorphous by X-ray diffraction [17]. Solid state nuclear magnetic resonance and vibrational spectroscopy further demonstrated that 0, 50 and 100%-strontium-strontium-substituted BG had predominantly Q2 silicate structures [17].

3.2. Dissolution ions studies

3.2.1. Ion release

The elemental concentrations of calcium, phosphorus, silicon and strontium released from BG into cell culture media are shown in Fig. 1. The dissolution of calcium into both RPMI 1640 and DMEM was dependent on BG composition, with decreasing media calcium concentration with increasing strontium substitution. The phosphorus concentration in RPMI 1640 changed little over the 4 h release period while in DMEM a general decrease in phosphorus concentration was observed for all BG compositions. The concentration of silicon in both RPMI and DMEM increased with dissolution time and was variable depending on culture media type and BG composition. The concentration of strontium was dependent on BG composition with increasing strontium substitution resulting in higher media strontium concentrations after 4 h.

3.2.2. Metabolic activity of cells

After 1 and 7 days in culture, there were no significant differences in the MTT activity of Saos-2 cells treated with BG dissolution ions compared to cells in standard culture medium (Fig. 2). After 14 and 28 days in culture, the MTT activity in cells treated with dissolution ions from all compositions of BG was significantly enhanced compared to controls. After 14 days in culture, MTT activity was significantly greater in Saos-2 cells treated with dissolution ions from 10, 50 and 100%-strontium-substituted BG compared to 0%-strontium-substituted BG. After 28 days in culture, cells treated with dissolution ions from 100% strontium-substituted BG had significantly higher MTT activity than that in any other group.

3.2.3. Formation of erosion pits by osteoclasts

RAW264.7 cells treated with RANKL formed erosion pits on CaP-coated slides (Fig. 3a) while those treated with RANKL and 1 μM pamidronate formed very few erosion pits (Fig. 3b). Mean erosion pit area, an indicator of osteoclast activity, decreased when RAW264.7 monocytes were treated with dissolution ions from BG in which an increasing proportion of calcium was substituted for with strontium (Fig. 3c). The correlation coefficient between strontium substitution and mean erosion pit area was $r^2 = 0.94$, which was statistically significant by Spearman's rho rank correlation.

3.2.4. Osteoclast differentiation and TRAP activity

RAW264.7 cells differentiated to large multinucleated osteoclasts in the presence of RANKL. Actin staining highlighted typical podosome belts in mature osteoclasts which appeared as prominent rings encasing multiple nuclei (Fig. 4a). Cultures treated with RANKL and 1 μM pamidronate (Fig. 4b) failed to form osteoclasts with distinctive podosome belts. After 4 days in culture, cells treated with dissolution ions from 100% strontium-substituted BG showed significantly less TRAP activity when compared to all other BG treated groups (Fig. 4c). After 6 days in culture, RAW264.7 treated with dissolution ions from 10%, 50% and 100% strontium-substituted BG all had significantly lower TRAP activity when compared to cells treated with dissolution ions from 0% strontium-substituted BG. The presence of 1 μM pamidronate significantly reduced total TRAP activity at all time points compared to all other groups. The presence of dissolution ions from all BG compositions, however, did not have an effect on cell number as no significant differences were detected between any groups at any time point (Fig. 4d). When TRAP activity was normalised to cell number, similar trends were noted although ANOVA determined them not to be significant with the exception that the group treated with 1 μM pamidronate had significantly lower TRAP activity per cell than any other group at any time point (Supplementary Fig. 1).

3.3. Bioactive glass discs studies

3.3.1. Total cell quantification

The total number of Saos-2 cells on BG discs increased over the two-week culture period for all BG compositions (Fig. 5a). After 24 h in culture, there were no significant differences between the number of cells on any BG disc composition. However, after 7 days in culture, there were significantly more cells on 100%-strontium-substituted BG discs than on 0%, and after 14 days in culture, there were significantly more cells on 50% and 100% strontium-substituted BG discs compared to either 0% or 10% strontium-substituted BG discs.

3.3.2. ALP activity

Saos-2 cells cultured on BG discs showed increased total ALP activity with increasing strontium substitution for calcium (Fig. 5b). There were no significant differences in total ALP per disc after 24 h in culture, but after 1 week, cells on 100% strontium-substituted BG discs had significantly higher total ALP activity than those on 0% or 10% strontium-substituted BG discs. After 2 weeks in culture, cells on BG discs with 50% or 100% strontium substitution had significantly higher total ALP activity than those on discs with 0% or 10% strontium substitution. This trend held when ALP activity was normalised per cell number as determined by LDH activity. There were no significant differences after 1 or 7 days in culture, but after 2 weeks, cells on BG discs containing 50% and 100% strontium substitution had significantly higher ALP activity per cell than those on 0% strontium-substituted BG discs (Supplementary Fig. 2).

3.3.3. SEM of osteoclasts

RAW264.7 monocytes cultured on standard BG discs differentiated to large cells with apico-basal polarisation, morphology typical of resorbing osteoclasts (Fig. 6). Osteoclasts with similar morphologies were observed adherent to the surfaces of all BG compositions by SEM (not shown). Many undifferentiated monocytes were also visible.

4. Discussion

Calcium has been reported to act as a network modifier in silicate glass systems such as BG. As strontium has a similar charge and ionic radius to calcium, when it is substituted into the glass network, it may play a similar role. The lower charge to size ratio of the strontium ion compared to the calcium ion (due to the slightly larger ionic radius of strontium), however, should create an expanded and more loosely cross-linked glass network, but not fundamentally alter the glass structure.

The release of calcium, phosphorus, silicon and strontium into cell culture medium during incubation with BG is complicated by ions already present in cell culture media, which themselves vary among media formulations. Our ICP-OES data show that despite its release from the BG, the calcium concentration in RPMI 1640 decreases and in DMEM stays fairly constant with incubation time. This is likely due to the formation of a CaP layer on the surface of the BG particles during incubation, which depletes the culture media of calcium [20]. This hypothesis is supported by the decrease...
in phosphorus concentration over time during incubation of BG in DMEM. The high concentration of phosphorus in RPMI 1640 (174 ppm) provides an excess available to form the CaP layer and so its concentration does not significantly diminish during incubation.

Silicon, which is thought to play a role in the cell-stimulating activities of BG dissolution ions due its essential role in bone formation [21], is released into culture media over time due to the breakup of the outer silica layers of the BG network [10]. While silicon release into simulated body fluid is reported to happen quickly (30 min–2 h), release into cell culture media proceeds more slowly [20], and although our data show that the silicon concentration in cell culture media increases with time for all BG compositions and in both media formulations, it does not reach its solubility limit (120 ppm in H2O). As expected, the substitution of strontium for calcium in BG results in increased levels of strontium in both RPMI 1640 and DMEM cell culture media. Taken together, these data suggest that the glass chemistry can be tailored to release an appropriate level of strontium and/or other ions depending on the application.

At early time points, the metabolic activity of Saos-2 cells treated with BG dissolution ions was not significantly different from that observed in cells treated with standard culture medium.

Fig. 1. Elemental concentrations of Ca, P, Si and Sr as determined by ICP-OES in cell culture media over 4 h incubation with BG particles in which 0, 10, 50 or 100% of the calcium was substituted for with strontium. Dissolution behaviour into (a) RPMI 1640 and (b) DMEM.
indicating that the dissolution products of all compositions of BG were non-cytotoxic. However, after 2 weeks in culture, dissolution ions from all formulations of BG enhanced total metabolic activity in Saos-2 cells compared to controls. This has been previously shown in primary human osteoblasts treated with 45S5 Bioglass\textsuperscript{®} dissolved in DMEM, which showed increased proliferation compared to controls\cite{22}. We also noted that MTT activity in cells treated with strontium-substituted BG was significantly enhanced compared to non-strontium-containing groups. This suggests that dissolution ions released from the strontium-substituted BG further enhance metabolic activity in Saos-2 beyond that caused by the presence of dissolution ions from standard BG. This is in agreement with previous studies which have shown that Sr\textsuperscript{2+} promotes osteoblast proliferation\cite{23} and suggests that strontium ions may act synergistically with other ions (most likely silicon) released from BG.

Treatting RAW264.7 monocytes with dissolution ions from BG with increasing strontium substitution reduced erosion pit area on CaP-coated glass slides. This suggests that the strontium ions either inhibit osteoclast differentiation or prevent mature osteoclasts from eroding the coating. SrR has been previously shown to both inhibit osteoclast differentiation and resorption activities \textit{in vitro} \cite{24}. Recent studies have suggested that modulation of osteoprotegerin and RANKL expression, known regulators of osteoclast activity and resorption, are responsible for this effect \cite{25}. Others, however, have shown that SrR inhibits osteoclast activity by preventing the formation of the ruffled border region and clear zone necessary for sealing and erosion pit formation \cite{5, 26}. Our data show that dissolution ions from strontium-containing BG did not prevent erosion pit formation to the same extent as the bisphosphonate pamidronate. Bisphosphonates act by disrupting the mevalonate pathway, disturbing osteoclast cytoskeleton.
Fig. 4. (a) Representative epifluorescense micrograph showing large multinucleated osteoclasts with typical podosome belts (arrows) in cultures of RAW264.7 mouse monocytes after 4 days treatment with RANKL and dissolution ions from 50% strontium-substituted BG. (b) Epifluorescence micrograph of RAW264.7 treated with RANKL and 1 µM pamidronate in which no multinucleated osteoclasts are visible. Red = phalloidin (actin), Blue = DAPI (nuclei). Scale bar in (a) and (b) is 200 µm. (c) Total TRAP activity (mean ± standard deviation) expressed as nmol p-nitrophenol liberated per minute in the presence of 20 mM tartrate in RAW264.7 differentiated in BG dissolution ion media or with 1 µM pamidronate (PAM). All cultures were supplemented with 20 ng/mL RANKL. Pamidronate significantly reduced total TRAP activity at all time points compared to all other groups (*). After 4 days, RAW264.7 treated with 100% strontium-substituted BG had significantly reduced TRAP activity compared to all other glass treated groups and controls treated with RANKL alone (CNT) (compared to CNT at same time point; † compared to 0%; ‡10%; ‡‡50%). After 6 days, cells treated with 10, 50 and 100% strontium-substituted BG had significantly lower TRAP activity when compared to 0% (‡). (d) Total number of cells in cultures of RAW264.7 monocytes treated with dissolution ions from BG or pamidronate. There were no significant differences between the number of cells detected in any group.
Substituting strontium for calcium in BG significantly decreased TRAP activity in cultures treated with their dissolution ions. ICP-OES demonstrated that DMEM cell culture medium treated with 100%-strontium-substituted BG had a strontium concentration of 84 ppm, which is similar to the concentration of strontium in cultures supplemented with 1 mM Sr²⁺ (88 ppm) (as either SrCl₂·6H₂O or SrR), which has also been shown to prevent osteoclast-mediated erosion of dentine slices [26] and apatite-coated matrices [5]. This level, however, is still higher than that in the serum of patients treated with SrR (0.12 mM Sr²⁺ or ~10 ppm [3]). Decreased TRAP activity, however, did not come as a result of cell death. While there is evidence of an apoptotic effect of SrR on osteoclasts [28,29], we could not detect significant differences in the number of cells in different groups at any time point. This is in agreement with studies which have shown that SrR does not affect attachment to or viability of osteoclasts on bone slices, but does reduce osteoclast differentiation and resorption activity [24]. Hurtel-Lemaire et al. have shown that SrR does induce osteoclast apoptosis, however, this was only evident at Sr²⁺ concentrations of 9 mM and higher, far more than that tested here and more than order of magnitude higher than that present in the serum of patients treated with SrR [29].

No addition of strontium to cell culture media by dissolution ions from BG reduced TRAP activity to the same extent as pamidronate. This is in keeping with results from a recent clinical trial that demonstrated a more subtle bone remodelling effect of SrR as compared to other osteoporosis treatments [30]. Parathyroid hormone (PTH) treatment enhances bone mineral density by both increasing bone formation and resorption. Anti-catabolic agents such as bisphosphonates, on the other hand, inhibit bone turnover, preserving the existing skeletal microarchitecture. Because of its mode of action, there has been concern that long-term treatment with bisphosphonates may 'freeze' bone, prohibiting normal repair processes. Recent reports of osteonecrosis in the jaw of patients treated with bisphosphonates seem to confirm this [31]. Neither PTH nor bisphosphonate treatments, however, address the lost bone remodelling balance inherent to osteoporosis. Bone regeneration therapies involving strontium may be preferred in this regard as they prevent osteoclast resorption without diminishing bone mineralisation and formation.

Strontium-substituted BG not only stimulated increased osteoblast metabolic activity and inhibited osteoclast differentiation and resorption via their dissolution ions, but also promoted osteoblast proliferation and ALP activity while directly in contact with cells. This is in agreement with studies on standard BG which have been shown to stimulate the expression of a number of osteogenic genes (reviewed in [32]), although the mechanism by which ions released from BG act on cells remains unclear. There is evidence that strontium's effect is mediated by cation-sensing receptors other than the calcium-sensing receptor (CaSR) [32,33,34]. This is supported by data demonstrating that neither calcium nor sodium ranelate had the same effects as their strontium counterpart [23,26]. However, this has been refuted by other studies which have demonstrated that strontium's effect is CaSR dependent [25,29], although an effect mediated by a combination of receptors cannot be ruled out.

Osteoclasts on BG discs assumed typical resorption morphologies, which was in contrast to non-resorbing morphologies noted in osteoclasts on tissue culture plastic. Previous studies have demonstrated that only when adherent to apatite do osteoclasts assume typical apico-basal polarisation and form sealing rings [35] suggesting that the BG discs examined in this study are sufficient to elicit a normal bone remodelling response. Our data also suggest that ions dissolved from BG are not sufficient on their own to
promote a resorption phenotype as osteoclasts cultured on tissue culture plastic in the presence of BG dissolution ions maintained flattened non-resorbing morphologies. This is in agreement with previous studies which have shown that microenvironmental cues alone do not trigger osteoclast polarisation and sealing zone formation [35].

5. Conclusions

Strontium can be substituted for calcium in BG, creating a biomaterial that increases osteoblast proliferation and ALP activity, and inhibits TRAP activity and osteoclast-mediated resorption of CaP films, in a similar manner to the osteoporosis drug SrR. As BG are a well-studied biomaterial system capable of controlled ion release and are deliverable as particulate, scaffolds or bulk material, substitution of strontium for calcium in BG may be an effective strategy for creating materials for bone repair/regeneration therapies.

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Appendix

Figures with essential colour discrimination. Part of Fig. 4 of this article is difficult to interpret in black and white. The full colour images can be found in the online version, at doi:10.1016/j.biomaterials.2010.01.121.

Appendix. Supplementary information

Supplementary data associated with this article can be found, in the online version, at doi:10.1016/j.biomaterials.2010.01.121.

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