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# ORIGINAL ARTICLE Quantitative rates of brain glucose metabolism distinguish minimally conscious from vegetative state patients

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The differentiation of the vegetative or unresponsive wakefulness syndrome (VS/UWS) from the minimally conscious state (MCS) is an important clinical issue. The cerebral metabolic rate of glucose (CMRglc) declines when consciousness is lost, and may reveal the residual cognitive function of these patients. However, no quantitative comparisons of cerebral glucose metabolism in VS/UWS and MCS have yet been reported. We calculated the regional and whole-brain CMRglc of 41 patients in the states of VS/UWS (n = 14), MCS (n = 21) or emergence from MCS (EMCS, n = 6), and healthy volunteers (n = 29). Global cortical CMRglc in VS/UWS and MCS averaged 42% and 55% of normal, respectively. Differences between VS/UWS and MCS were most pronounced in the frontoparietal cortex, at 42% and 60% of normal. In brainstem and thalamus, metabolism declined equally in the two conditions. In EMCS, metabolic rates were indistinguishable from those of MCS. Ordinal logistic regression predicted that patients are likely to emerge into MCS at CMRglc above 45% of normal. Receiver-operating characteristics showed that patients in MCS and VS/UWS can be differentiated with 82% accuracy, based on cortical metabolism. Together these results reveal a significant correlation between whole-brain energy metabolism and level of consciousness, suggesting that quantitative values of CMRglc reveal consciousness in severely brain-injured patients.

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### INTRODUCTION

Disorder of consciousness (DOC) is a frequent complication of severe brain injury. The diagnosis covers several pathologic states, characterized by diminished responsiveness at the bedside. Among the patients with DOC, those in the vegetative state (VS) or, as recently proposed, in the unresponsive wakefulness syndrome (UWS), retain arousal (i.e., eye opening), but exhibit no behavior indicative of awareness.<sup>1</sup> In the minimally conscious state (MCS), patients display different but reproducible signs of awareness, but are unable to communicate functionally.<sup>2</sup> By convention, emergence from the MCS (EMCS) occurs when patients regain a capacity for functional communication or object use.<sup>2</sup> The differentiation among the states of VS/UWS, MCS, and EMCS is a serious challenge to society and to the clinic. In these conditions, quantitative molecular neuroimaging is a promising complement to bedside assessment,<sup>3</sup> because DOC is associated with widespread reductions of cerebral energy metabolism.<sup>4</sup> The energy metabolism of the brain relies on uninterrupted glucose consumption, which is measured with positron emission tomography (PET) with [<sup>18</sup>F]fluorodeoxyglucose (FDG). We have previously shown that analysis of regional metabolic patterns on global mean-normalized FDG-PET scans provide a strong differential diagnostic tool in DOC.<sup>5</sup> This method, however, only takes relative regional differences of brain metabolism into account, with no assessment of absolute metabolic differences among the conditions. Important information, such as global cerebral metabolism, is lost in the normalization process, which in some cases leads to false diagnosis. It is necessary to quantitatively determine metabolism to improve the reliability of the FDG-PET diagnostic approach to DOC. As patients in VS/UWS, MCS, and EMCS occupy a zone of transition between the states of full consciousness and unconsciousness, they also afford a unique, if unfortunate, opportunity to investigate the neurobiology of conscious awareness.

During loss of consciousness, cerebral metabolic rates of glucose (CMRglc) fall to 50% of normal or less.<sup>4</sup> In previous studies, reported decreases of CMRglc to 40% to 50% of normal in patients in the acute phase of VS/UWS declined further to 30% to

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40% in transition to subacute and chronic stages.<sup>6–8</sup> However, it remains unclear whether the metabolic changes correlate directly with the level of consciousness, or whether they rather reflect the extent of neuronal damage at the onset of the condition. Gjedde<sup>9</sup> argued that incrementally increasing levels of consciousness appear to be associated with a stepwise doubling of rates of energy metabolism. He proposed that the transition among conscious states is linked to metabolic phase transitions.<sup>9,10</sup> Thus. uniformly high baseline energy metabolic rates appear to be necessary to support full consciousness, as argued by Shulman.<sup>10</sup> By inference, MCS would be associated with higher CMRglc than VS/UWS. A certain proportion of the brain's energy budget is reserved for cellular homeostatic processes at an isoelectric baseline of electroencephalographic activity.<sup>11</sup> Here, we argue that the transition from VS/UWS to MCS must occur with increments of whole-brain energy metabolism relative to this isoelectric baseline. A test of this hypothesis has not yet been reported, as no group study directly assessed the quantitative differences of CMRglc among patients in VS/UWS and MCS. Neither did previous studies of CMRalc with PET of FDG in VS/UWS address the guestion of the extent to which the metabolic requirements of consciousness are global, or whether regional increases confined to specific brain regions are sufficient to restore consciousness. Previous studies indicated that areas associated with conscious activity include arousal centers in the brainstem, and a set of cortical regions including the frontoparietal network and precuneus<sup>12</sup> that belong to a global workspace of consciousness.<sup>13</sup> The authors argued that these regions depend on an ascending arousal system that interacts with 'default mode' and executive control networks, which respectively are held to subserve internal or introspective,<sup>14</sup> and external or extrospective,<sup>15,16</sup> awareness. Other studies alternatively suggest that central thalamic nuclei serve to connect the ascending arousal system to the entire cortex supporting awareness, and to drive the cortical activity necessary for consciousness.<sup>10,17</sup>

In the present study, we test the hypothesis of a threshold at 50% of normal whole-brain or cortical CMRglc values for the transitions of patients among the VS/UWS, MCS, and EMCS states, in relation to healthy controls. We expect patients in the conditions of MCS and EMCS to have significantly higher cortical, thalamic, and brainstem metabolic rates, than patients in the condition of VS/UWS. In line with previous studies,<sup>4,18</sup> we expect these differences to be most pronounced in the frontoparietal associative cortices and the precuneus, but to remain small compared with the average whole-brain differences. We further hypothesize that patients in MCS and EMCS do not differ with respect to CMRglc, as both groups have undergone transition to minimal awareness, although with differences of cognitive capacity.<sup>19</sup>

#### MATERIALS AND METHODS

### Patients

Our study population was a convenience sample of patients diagnosed with the Coma Recovery Scale-Revised (CRS-R) as being in VS/UWS, MCS, or EMCS. All patients were admitted to the Liège University Hospital in the period 2010 to 2012. The population comprised 41 patients (mean age: 41 ± 18 years; 26 males), 14 in VS/UWS, 21 in MCS, and 6 in EMCS. Of these, 15 patients had traumatic and 26 patients had nontraumatic etiologies (i.e., cardiac arrest, stroke, hemorrhage, infection, and metabolic disorders). Average duration since insult was 27 months (range: 24 days to 9 years). We also included 29 healthy controls with no history of neurologic disorders (mean age:  $44 \pm 16$  years; 19 males). Table 1 summarizes the patient data. The study was conducted in accordance with the Helsinki Protocol, and approved by the Ethics Committee of the University Hospital of Liège. All healthy participants, and legal representative of all patients gave written informed consent.

Diagnosis N Age Male Months since onset, Traumatic (mean ± s.d.) mean (range) etiology					
VS/UWS	14	45 (±16)	8	21 (16 days-8 years)	1
MCS	21	33 (±15)	18	34 (10 days-9 years)	11
EMCS	6	30 (±15)	5	12 (75 days-3 years)	3
Total	41	39 (±16)	31	27 (10 days–9 years)	15
EMCS, emergence from minimally conscious state; MCS, minimally conscious state; VS/UWS, vegetative state/unresponsive wakefulness syndrome					

#### Behavioral Diagnosis

The CRS-R was used to define the clinical diagnosis, as the most sensitive tool for discriminating low awareness levels.<sup>20,21</sup> The CRS-R has six subscales, including auditory, visual, motor and oromotor/verbal functions, communication, and level of arousal (Supplementary Table 1). Trained neuropsychologists conducted the CRS-R assessment at least once a day over 5 days, and the best result obtained was used to determine the diagnosis.

#### PET Data Acquisition

We acquired all PET data with Gemini PET-computed tomography (Philips Medical Systems) at the University Hospital of Liège. Following intravenous injection of 185 to 370 MBq FDG, we recorded a single PET frame for 12 minutes, after circulation of the tracer for at least 30 minutes. We maintained the patients awake during the uptake period. The images were corrected for attenuation using X-ray computed tomography, as well as for random scatter and physical decay.

#### Calculation of Glucose Metabolism

Quantitative determination of CMRglc in patients with DOC is an important methodological challenge. PET imaging of FDG with arterial blood sampling is ethically tenuous, as the patients cannot give consent to the prolonged invasive procedure.<sup>3</sup> We therefore quantified CMRglc with Sokoloff's autoradiographic method,<sup>22</sup> using a standard arterial input function obtained from 10 healthy volunteers.<sup>23,24</sup> Plasma glucose levels were obtained from a single cutaneous blood sample immediately before image acquisition. For the calculation, we used the glucose transfer coefficients and lumped constant of 0.61 reported by Kuwabara and Gjedde.<sup>25</sup> The use of standardized arterial input curves assumes corresponding lumped constants and input function shapes for healthy subjects and patients with brain injury. It further assumes similar plasma glucose levels in all subjects during image acquisition, a condition that was met (Supplementary Table 2). Sokoloff's autoradiographic method makes primary use of the recorded radioactivity, to which the transfer constants  $K_{1}$ ,  $k_{2}$ , and  $k_{3}$  make a minimal contribution at late times after tracer injection. Effects of pathologic conditions such as low cerebral blood flow on the magnitude of these constants, therefore have a negligible effect on the calculated value of CMRglc.<sup>26</sup>

#### PET Image Processing

We coregistered the images in MNI-space, using the Orderless Mutual Information framework.<sup>27</sup> This registration method is developed for large spatial deformations, and is more robust to brain atrophy and focal lesions than standard coregistration methods.

We generated average group images of the VS/UWS, MCS, and healthy controls. We identified absolute group differences by pairwise subtraction of average metabolic maps. We performed whole-brain voxel-wise comparison of subjects in MCS and VS/UWS with statistical parametric mapping (SPM 8, implemented in MATLAB), after smoothing with a 14 mm FWHM kernel. To avoid focal lesions affecting the comparison, voxels with intensity < 0.5 of image maximum were masked out. We contrasted the diagnostic groups in a pairwise manner to identify sites with significant differences among the conditions.

We used the Harvard-Oxford atlas to parcellate the brains into discrete regions.<sup>28</sup> All cortical regions were merged to create a whole-brain cortical mask. To assess activity in the areas of greatest difference between

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subjects in MCS and VS/UWS, we constructed a regional mask corresponding to the SPM difference map of the contrast MCS>VS/UWS, at P < 0.005 uncorrected. Due to ex-vacuo hydrocephalus, the coregistration procedure failed to align the thalami perfectly. We therefore generated a thalamic region of interest by manually placing a sphere ( $\emptyset = 1$  cm) centered on the core of the thalamus. Median metabolic rates were extracted for all regions. We included the regional uptake values of the entire cortex, precuneus, maximum difference mask, thalamus, and brainstem for further statistical analysis. The remaining regional values are provided in Supplementary Table 3.

#### Statistical Analysis

We determined group differences of rCMRglc using the general linear model, with etiology and time since onset as covariates. We used the Wilcoxon rank-sum tests to assess the significance of pairwise regional differences among VS/UWS, MCS, and healthy controls. We also determined differences in regional metabolic rates between MCS and EMCS.

For each region, we further assessed correlations with the CRS-R score and the arousal subscore, both the overall average and the score on the day of PET scan, using the general linear model. To test whether CMRglc values reflect the patient status at the specific time of scanning, we further correlated the rCMRglc values of patients in MCS and EMCS with their CRS-R diagnosis (EMCS, MCS, or VS/UWS) on the day of image acquisition.

To identify the cortical metabolic threshold over which patients are more likely to be in MCS than in VS/UWS, we performed an ordinal logistic regression by patient group (MCS, VS/UWS, or control), on the overall cortical metabolic rates and the metabolic rates within the maximum difference mask.

We assessed the variability of cortical metabolism within subjects, by calculating standard deviation of voxel-wise uptake values within the cortical mask. We calculated the energy turnover supporting synaptic transmission by subtracting the metabolic background associated with cellular homeostatic processes (0.0375  $\mu$ mol/g per minute<sup>29</sup>). This value corresponds to the average cortical glucose metabolism associated with isoelectric electroencephalographic activity level. We subtracted this constant metabolic background from the value determined in each voxel of each image.

To examine the possibility of differentiating patients in VS/UWS and MCS on the basid of their values of CMRglc, we plotted receiver-operating characteristics (ROC) curves for rCMRglc, as well as for the cortical voxelwise variability. We thus used the CRS-R as diagnostic reference, and plotted the ratio of correctly classified patients at increasing metabolic

VS/UWS

cutoff points of discrimination between the conditions. As we tested for the presence of minimal consciousness, we assigned a correct classification of MCS as a true positive. Posing no clinical diagnostic problems, patients in EMCS and controls were not included in this test. We used the area under the ROC curve as a measure of diagnostic accuracy. We further plotted the likelihood ratio of being MCS versus VS/UWS, for increasing thresholds of rCMRglc.

# RESULTS

#### Global Glucose Metabolism

All patients had globally reduced cerebral metabolic rates of glucose, relative to healthy controls, but the MCS patients had higher rates of metabolism than patients in VS/UWS in all cortical areas (Figure 1). In the voxel-wise comparison, the regions with the most significant differences belonged to the primary and associative sensory (visual, auditory, and somatosensory) and motor areas bilaterally (P < 0.001 uncorrected, Figure 2). With a less severe statistical threshold of P < 0.005 (uncorrected), we observed differences between patients in MCS and VS/UWS in a larger frontoparietal region that included the fronto-, temporo-, and occipito-parietal junctions. We subsequently refer to this region as the 'maximum difference map'. No voxels survived correction for family-wise error. No subcortical regions had significant differences, even at P < 0.005 (uncorrected, Figure 2).

Median cortical glucose metabolic rates averaged 42% of normal in VS/UWS patients, 55% of normal in MCS patients, and 53% of normal in EMCS patients (Table 2, Figure 3). The group differences were significant, at P < 0.022 (VS/UWS < MCS), P < 0.001 (VS/UWS < controls), P < 0.001 (MCS < controls), and P < 0.001 (EMCS < controls), respectively. Differences between MCS and EMCS were not significant (P > 0.1).

#### Regional Glucose Metabolism

Fully conscious subjects

Median glucose metabolic rates within the maximum difference map (P < 0.005) averaged 42% of normal in VS/UWS, 60% of normal in MCS, and 55% of normal in EMCS (Table 2, Figure 3). Group differences were significant at P < 0.001 (VS/UWS < MCS), P < 0.001 (VS/UWS < controls), P < 0.001 (MCS < controls), and

0.3



MCS

**Figure 1.** Average CMRglc (µmoL/g per minute) by condition (14 patients in VS/UWS, 21 patients in MCS, and 29 fully conscious controls). CMRglc, cerebral metabolic rate of glucose; MCS, minimally conscious state; VS/UWS, vegetative state/unresponsive wakefulness syndrome.



**Figure 2.** Metabolic differences between 14 patients in VS/UWS and 21 patients in MCS. Left: subtraction of average VS/UWS image from average MCS image. Right: areas where activity in MCS is significantly higher than in VS/UWS, at P < 0.001 uncorrected (light blue) and P < 0.005 uncorrected (dark blue). MCS, minimally conscious state; VS/UWS, vegetative state/unresponsive wakefulness syndrome.

Table 2. Average regional metabolic rates of glucose					
Diagnosis	Whole cortex (µmoL/g per minute)±s.d.	Precuneus (μmol/g per minute)±s.d.	Maximum difference map (µmol/g per minute)±s.d.	Thalamus (μmol/g per minute)±s.d.	Brainstem (μmol/g per minute)±s.d.
VS/UWS	0.127 (±0.025)	0.130 (±0.026)	0.125 (±0.023)	0.142 (±0.026)	0.149 (±0.032)
MCS	0.167 (±0.05)	0.177 (±0.052)	0.178 (±0.049)	0.154 (±0.040)	0.16 (±0.055)
EMCS	0.158 (±0.035)	0.170 (±0.045)	0.164 (±0.033)	0.136 (±0.041)	0.155 (±0.043)
Control	0.300 (±0.0306)	0.343 (( <u>+</u> 0.039)	0.296 (±0.032)	0.365 ( <u>+</u> 0.046)	0.23 (±0.03)
EMCS, emergence from minimally conscious state; MCS, minimally conscious state; VS/UWS, vegetative state/unresponsive wakefulness syndrome.					

P < 0.001 (EMCS < controls), respectively. Differences between MCS and EMCS were not significant (P > 0.1).

Precuneal glucose metabolic rates averaged 38% of normal in VS/UWS, 51% of normal in MCS, and 50% of normal in EMCS (Table 2, Figure 3). Group differences were significant at P < 0.002 (VS/UWS < MCS), P < 0.001 (VS/UWS < controls), P < 0.001 (MCS < controls), P < 0.001 (MCS < controls), and P < 0.001 (EMCS < controls), respectively. Differences between MCS and EMCS were not significant (P > 0.1).

Thalamic glucose metabolic rates averaged 39% of normal in VS/UWS, 42% of normal in MCS and 37% of normal in EMCS (Table 2, Figure 3). No significant differences existed between thalamic metabolic rates of MCS and VS/UWS subjects (P < 0.1), or between MCS and EMCS (P < 0.1). All patients had decreased metabolism than controls, at P < 0.001 (VS/UWS < controls), P < 0.001 (MCS < controls) and P < 0.001 (EMCS < controls).

Brainstem glucose metabolic rates were 65% of normal in VS/UWS, 70% of normal in MCS, and 67% of normal in EMCS (Table 2, Figure 3). No significant differences appeared between brainstem metabolic rates of MCS and VS/UWS patients (P>0.1), or between MCS and EMCS patients (P>0.1). All patients had decreased metabolism than controls, at P < 0.001 (VS/UWS < controls), P < 0.001 (MCS < controls); and P < 0.001 (EMCS < controls).

We found no significant correlations between rCMRglc reductions and time since onset, etiology, or age for any group in any of the selected regions. Measures of rCMRglc did not correlate with CRS-R or arousal subscores, as measured before or on the day of PET (see Supplementary Table 3 for individual scores). Average within-subject voxel-wise variances of cortical metabolism were 0.029 s.d. in VS/UWS, 0.047 s.d. in MCS, 0.040 s.d. in EMCS, and 0.068 s.d. in healthy controls (Table 3, Figure 3). The difference in cortical CMRglc variance between VS/UWS and MCS was significant at P < 0.001. The difference between MCS and EMCS was not significant (P > 0.1). All patients had decreased variability than controls, at P < 0.001 (VS/UWS < controls), P < 0.001 (MCS < controls) and P < 0.001 (EMCS < controls).

Ordinal logistic regression showed that the likelihood of diagnosis shifted from VS/UWS to MCS at a threshold of metabolic rate of 44% of normal (0.132  $\mu$ mol/g per minute) in the entire cortex, and above 46% of normal (0.138  $\mu$ mol/g per minute) within the maximum difference map. Eight MCS patients had CRS-R scores corresponding to a status of VS/UWS on the day of the PET. Average cortical CMRglc values of these patients (0.175  $\mu$ mol/g per minute) matched that of the 13 patients clinically in MCS at image acquisition (0.162  $\mu$ mol/g per minute; see Supplementary Table 3 for individual patient data).

The glucose consumption required for tissue homeostasis, without cellular communication, is ~12.5% of normal cortical metabolism.<sup>29</sup> To assess the energy turnover associated with synaptic firing in each group, we therefore subtracted the value of this threshold of 0.0375  $\mu$ mol/g per minute for each patient. The results are consistent with maintained activity above isoelectricity at average levels of 34% of normal in VS/UWS, 49% of normal in MCS, and 47% in EMCS (Table 3).

The ROC analysis provided an area under the ROC curve of 0.73 for the entire cortex, 0.74 for the precuneus, 0.87 for the maximum

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**Figure 3.** Regional cerebral metabolic rates of glucose ( $\mu$ mol/g per minute). Top left: median cortical CMRglc. Top middle: median precuneal CMRglc. Top right: median CMRglc within mask of areas with significant differences between MCS and VS/UWS at P < 0.005. Bottom left: median thalamic CMRglc. Bottom middle: median brainstem CMRglc. Bottom right: average voxel-wise variability in the cortex. CMRglc, cerebral metabolic rate of glucose; MCS, minimally conscious state; VS/UWS, vegetative state/unresponsive wakefulness syndrome.

Table 3. Synaptic contribution and variance of cortical metabolism				
Diagnosis	Cortical synaptic activity (µmol/g per minute)±s.d.	Mean within-subject voxel-wise s.d. of cortical metabolism (μmol/g per minute)		
VS/UWS	0.090 (±0.025)	0.029		
MCS	0.129 (±0.05)	0.047		
EMCS	0.123 (±0.035)	0.040		
Control	0.262 (±0.031)	0.068		
EMCS, emergence from minimally conscious state; MCS, minimally conscious state; VS/UWS, vegetative state/unresponsive wakefulness syndrome.				

difference map (i.e., frontoparietal cortex), and 0.86 for the cortical variability of metabolism (Figure 4, Table 4). The highest classification rate achieved was 83% (using the cortical variability of metabolism; Table 4). The likelihood of being in MCS rather than VS/UWS increased with increasing CMRglc (Figure 4). We plotted no ROC curves or likelihood ratios of consciousness for thalamus and brainstem, as we found no significant metabolic differences between VS/UWS and MCS in these regions.

## DISCUSSION

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We determined regional and whole-brain values of CMRglc of 41 patients in VS/UWS, MCS, or EMCS, with PET of the glucose metabolism tracer FDG. We found a significant global decline in cerebral metabolism in severely brain-injured patients compared with healthy controls. The patients in MCS had significantly higher metabolic rates (55% of normal) than the VS/UWS patients (42% of normal) in all cortical regions. The differences of regional CMRglc between MCS and VS/UWS were most pronounced in the sensory, frontoparietal, and motor cortices, whereas no subcortical structures were differentially affected. As expected, we found no significant metabolic differences between the MCS and EMCS patients.

The findings show that states of unconsciousness after severe brain injury are associated with a global decrease of CMRglc within the range of 40% to 50% of normal resting activity in fully conscious individuals. Similar decreases of CMRglc occur in anesthesia induced by any of a wide range of pharmacological agents,<sup>30–32</sup> as well as in deep sleep,<sup>33</sup> and coma. The results are consistent with the hypothesis that a brain energy turnover rate above a certain threshold is necessary for support of consciousness.<sup>9,10</sup> Results of previous studies have implicated impairments of the frontoparietal and precuneal cortex, thalamus, and brainstem in states of unconsciousness. The present results indicate that cerebral metabolic differences among the patient groups are global, but most pronounced in the frontoparietal and precuneal cortices, and with no specific involvement of the thalamus and brainstem.

#### Global Decline of Metabolism

The overall cortical CMRglc was lower in patients than in healthy control subjects, but significantly higher in MCS than in VS/UWS patients. Metabolism did not differ significantly between the patient groups of MCS and EMCS. The results imply that the cortical rate of metabolism is an important determinant of whether a patient is unconscious or retains some degree of awareness. Etiology, time since insult, and CRS-R scores, and arousal subscores did not correlate with the global metabolism, indicating that the metabolic differences were probably associated with level of consciousness rather than with possible confounding factors. It is thus reasonable for us to conclude that a tight correlation exists between level of conscious awareness and energy turnover in the brain. However, we observed a significant overlap of individual cortical metabolism values between the MCS and VS/UWS patients. Although few MCS patients had cortical metabolic rates below the VS/UWS average, and no VS/ UWS patients had metabolic rates above the MCS average, a majority of the patients had metabolic rates between the two limits. Thus this finding is consistent with a gradual transition between the states. The ordinal logistic regression indicated a threshold of cortical



**Figure 4.** Ability to differentiate VS/UWS from MCS, based on rCMRglc and cortical variance. Left: receiver-operating characteristic (ROC) plots of metabolism within the entire cortex, precuneus, frontoparietal cortex (areas with significant differences between MCS and VS/UWS at P < 0.005), and the cortical variance. True positive fraction (TPF) = sensitivity to MCS, false positive fraction (FPF) = 1 – specificity to MCS. Right: likelihood ratio of being MCS rather than VS/UWS at increasing metabolic thresholds. A gradual increase is seen above 0.135  $\mu$ mol/g per minute for all regions corresponding to 45% of normal cortical CMRglc. CMRglc, cerebral metabolic rate of glucose; MCS, minimally conscious state; VS/UWS, vegetative state/unresponsive wakefulness syndrome.

Table 4.	Diagnostic precision of regional metabolic measures			
Regional	measure	AUROC (95% CI)	Best classification rate (%)	
CMRglc,	cortex	0.73 (0.56–0.9)	74	
CMRglc, differen	maximum ce map	0.87 (0.76–0.99)	80	
CMRglc,	precuneus	0.74 (0.66–0.95)	74	
Cortical	variance	0.86 (0.73–0.99)	83	
AUROC, area under the receiver operating characteristic curve; CI, confi-				

dence interval; CMRglc, cerebral metabolic rate of glucose.

CMRglc near 45% of the normal average, below which no patient is likely to undergo transition into MCS. The overlap also implies that elevated cortical metabolism may be a necessary but not sufficient condition for emergence of consciousness.<sup>10</sup> Interestingly, the seven MCS patients who were clinically unresponsive on the day of the PET had CMRglc values that matched those of the responsive patients in MCS at image acquisition. The match further suggests that energy turnover enables awareness, but does not determine the specific level of consciousness expressed at the time of tomography. This hypothesis requires testing in a larger patient sample, however.

## Metabolism in Support of Synaptic Transmission

Considering the presumed fundamental difference between the states (MCS and VS/UWS), the overall difference of CMRglc was surprisingly small. The modest difference may in part reflect the action of cellular homeostatic processes, which account for a relatively large portion of the overall energy budget when neurotransmission is inactive or inefficient. As the basic homeostatic requirements are held to be similar in MCS and VS/UWS, cognitive functional differences between MCS and VS/UWS may take up a relatively small part of the overall metabolism. In fully conscious subjects, close to 90% of the overall energy turnover of the brain in terms of oxidative glucose metabolism is dedicated to synaptic activity.<sup>11</sup> Close readings of studies that replicate the findings of Sibson *et al*<sup>11,29</sup> suggest that the static baseline activity accounts for approximately one-eighth of the normal cortical metabolism (0.0375  $\mu$ mol/g per minute by inference from the

present data). Subtraction of the isoelectricity baseline from the total cortical metabolism thus provides an approximation of the level of energy turnover associated with synaptic firing in each patient. According to this calculation, on average, neurotransmission in VS/UWS drew upon no more than 34% of normal average, whereas neurotransmission in MCS drew upon metabolic rates close to 50% of the normal average. The overall transmission in MCS patients thus is markedly higher than in VS/UWS patients. Considering the total lack of cognitive responsiveness in VS/UWS, the level of basic noncognitive spontaneous neural activity inferred from the metabolism is remarkably high. The results show that the emergence of conscious awareness correlates nonlinearly with the level of metabolism, and they support the hypothesis that a decisive phase shift occurs at an energy turnover of  $\sim 45\%$  of normal average, at which it enables the specific neuronal conditions necessary for the rise of consciousness.

## Cerebral Energetics and Cortical Connectivity

Loss of consciousness is associated with widespread loss of cortical connectivity. Particularly, studies of DOC, sleep, and anesthesia reveal decreased global connectivity,<sup>34</sup> and decreased default mode network connectivity,<sup>14</sup> decreased thalamocortical connectivity,<sup>35,36</sup> and decreased feedback connectivity, between frontal and temporal lobes.<sup>37</sup> Although disruption of connectivity appears to be a key feature of DOC, the underlying pathologic mechanisms are not clear.<sup>3</sup> The concurrent observations of metabolic decrease and disrupted connectivity in all states of diminished consciousness suggest a common physiologic ground.

Animal studies show that high neuronal cerebral metabolic rates of oxygen (CMRO<sub>2</sub> $\approx$ 80% to 90% of normal) are consistent with high frequency neuronal firing and widespread cortical integration of stimuli. At decreased baseline energetics (CMRO<sub>2</sub> below 50% of normal), neuronal firing rates shift toward low frequencies, and long-range cortical connectivity declines.<sup>11,38</sup> The findings support the purported link between neuronal energetics and cerebral connectivity.

With average cortical CMRglc values of ~40% and 'synaptic' energetics at 34% of normal, VS/UWS patients may be in a state of low baseline energy turnover in cortex. On the basis of Maandag *et al*,<sup>38</sup> the neuronal activity of these patients would be dominated by low-frequency ensembles, which are not reflective of wide-spread cortical connectivity. The absence is consistent with

electroencephalographic evidence in VS/UWS of increased amplitude in lower frequency bands (delta and theta) and decreased activity at higher frequencies (beta and gamma).<sup>39,40</sup> In turn, MCS patients may approach an intermediate energy state, with energy turnover rates supporting a gradual transition towards normal neuronal activity,<sup>40,41</sup> enabling long-range cortical connectivity and rise of conscious awareness. The arguments support the hypothesis of globally decreased cortical energy turnover below 45% of normal that are incompatible with conscious awareness.

## Regional Metabolic Contributions to Level of Consciousness

Loss of consciousness is evidently associated with a large global decline of metabolism. However, we also observed regional variations relative to the global effect, which allowed inferences about the specific pathologic anatomy of DOC.

It is commonly held that DOC patients are 'awake but unaware' with preserved arousal systems, but impaired awareness.<sup>3,42</sup> Although several studies confirm relatively preserved brainstem metabolism in VS/UWS patients,<sup>3,4,42</sup> the present findings reveal brainstem metabolic declines to 60% to 70% of normal in all patient groups. Although brainstem metabolism is less affected than cortical metabolism, the findings clearly indicate impaired ascending arousal that may explain the fluctuations of wakefulness observed in DOC.<sup>1,2</sup>

The voxel-wise comparisons revealed that metabolic rates in the primary sensorimotor areas, adjacent frontoparietal regions, and precuneus, distinguish MCS from VS/UWS. However, the high interindividual metabolic variability prohibited robust inferences about voxel-wise regional differences. Nonetheless, average activity within the frontoparietal regions (the maximum difference map MCS > VS/UWS) was markedly higher in MCS (60% of normal) than in VS/UWS (42% of normal), in support of a critical role of the associative frontoparietal cortices in DOC.<sup>18,43</sup> The precuneus and adjacent posterior cingulate cortex are believed to integrate input from these frontoparietal awareness networks.44 Thus, the precuneal activity appeared to closely match the general frontoparietal CRMglc rates. It has been proposed that preserved metabolic rates in the precuneus differentiate MCS from VS/UWS, and axonal regrowth in the precuneus has been seen as the driving mechanism of recovery from MCS.<sup>45</sup> However, as several of the MCS patients had precuneal rCMRglc values in the same range as the VS/UWS population, preserved precuneal activity does not appear to be pathognomonic for individual MCS patients.

There is evidence both *in vivo*<sup>46</sup> and postmortem<sup>47</sup> that thalamic injury is a fundamental pathogenic mechanism in DOC. Reestablishment of thalamocortical connectivity has been proposed as the main driver of recovery of consciousness,<sup>36</sup> either through direct excitatory input to the cortex,<sup>17,48</sup> or by temporal synchronization of corticocortical interactions that enable phenomenal awareness.<sup>49</sup> Although thalamic metabolism was strongly reduced in all patient groups, it did not differentiate MCS from VS/UWS, implying that it is not the single most important determinant of level of consciousness in DOC. Further studies of connectivity may resolve this issue. Thus, the most important distinctions between MCS and VS/UWS appear restricted to the cerebral cortex, in particular the frontoparietal and precuneal regions. Even in the areas with the most significant differences between MCS and VS/UWS, the average regional measures of metabolism did not allow clear distinction between the states of consciousness of individuals, possibly because the average values of rates of regional metabolism are inadequate measures of small functional differences within larger networks. MCS and EMCS patients had large variances of voxel-wise FDG uptake values across the cortex. It is possible that these patients had clusters of activity sufficient to support consciousness in small

areas, while activity averaged across large regions remained low. In contrast, the distribution of cortical activity in VS/UWS was uniform, with little voxel-wise variability. By inference, VS/UWS patients have uniformly low metabolism in all areas of the brain. with no regions of normal metabolism. The existence of small functionally intact cortical islands within sensory (input), frontoparietal (awareness), and motor (output) networks, could be pathognomonic of the MCS condition.<sup>4</sup>

# **Clinical Implications**

The results show that measures of CMRglc may differentiate patients in MCS from patients in VS/UWS. The 'optimal' metabolic cutoff to differentiate the conditions depends on the relative importance assigned to false diagnoses of VS/UWS and MCS, respectively. We therefore could not determine unequivocal measures of sensitivity and specificity. The individual cutoff points of the ROC curves show that correct classification rates of up to 83% can be achieved on the basis of cortical metabolism alone. As predicted from the ordinal logistic regression, the probability of being conscious increases dramatically at metabolic rates >45% of normal cortical levels for all cortical regions. We previously showed that pattern analysis of normalized regional metabolism has strong diagnostic utility.<sup>5</sup> As the absolute metabolic values provide important additional information, clinical diagnostic methods should be developed that take both absolute measures of metabolism and interregional relations into account. The CMRglc measures do not provide information of the specific cognitive capacity of the patients, and should thus be used chiefly as a means to discriminate conscious from unconscious patients. The method has the advantage of being independent of language and motor skills, and it can supplement bedside assessments, particularly in cases where aphasia, cognitive deficits or paralysis challenges communication-dependent diagnostic methods. It also presents a reliable alternative to activation-based neuroimaging paradigms, such as mental imagery during functional MRI, which also depends on relatively preserved cognition and language comprehension. A particular application could be identification of patients suffering from locked-in-syndrome, characterized by low brainstem metabolism, but relatively preserved cortical metabolism.<sup>6</sup> FDG-PET measures cellular activity, and only indirectly reveals the extent of neuronal damage. Future studies with tracers of neuronal integrity, such as 11C-flumazenil, could provide a more direct measure of preserved neuronal tissue, to support clinical prognosis.

# CONCLUSION

The present findings reveal a strong correlation between overall cortical energy turnover and level of consciousness. A high baseline energy turnover may be a necessary, if not sufficient, condition for the rise of conscious awareness, by enabling longdistance connectivity across the cortex. VS/UWS patients retained a surprisingly high level of metabolism, in the range known to be associated with spontaneous synaptic activity, implying that consciousness correlates nonlinearly with neuronal work. The findings suggest that a physiologic phase shift occurs at an energy turnover just below 50% of normal, where it enables the rise of conscious awareness. Conscious individuals had significantly higher variability of cortical metabolism than unconscious patients. Thus islands of preserved activity across the cortex may be pathognomonic for the MCS. We further show that absolute cortical metabolic activity may be utilized as a clinical tool to help disentangle patients in MCS and VS/UWS.

# DISCLOSURE/CONFLICT OF INTEREST

The authors declare no conflict of interest.

# REFERENCES

- 1 Medical aspects of the persistent vegetative state (1). The Multi-Society Task Force on PVS. *N Engl J Med* 1994; **330**: 1499–1508.
- 2 Giacino JT, Ashwal S, Childs N, Cranford R, Jennett B, Katz DI *et al.* The minimally conscious state: definition and diagnostic criteria. *Neurology* 2002; **58**: 349–353.
- 3 Laureys S, Schiff ND. Coma and consciousness: paradigms (re)framed by neuroimaging. *Neuroimage* 2012; 61: 478–491.
- 4 Laureys S, Owen AM, Schiff ND. Brain function in coma, vegetative state, and related disorders. *Lancet Neurol* 2004; **3**: 537–546.
- 5 Stender J, Gosseries O, Charland-Verville V, Vanhaudenhuyse A, Demertzi A, Chatelle C et al. Diagnostic precision of PET imaging and functional MRIin disorders of consciousness: a clinical validation study. *Lancet* 2014; **384**: 514–522.
- 6 Levy DE, Sidtis JJ, Rottenberg DA, Jarden JO, Strother SC, Dhawan V *et al.* Differences in cerebral blood flow and glucose utilization in vegetative versus locked-in patients. *Ann Neurol* 1987; **22**: 673–682.
- 7 Rudolf J, Ghaemi M, Ghaemi M, Haupt WF, Szelies B, Heiss WD. Cerebral glucose metabolism in acute and persistent vegetative state. *J Neurosurg Anesthesiol* 1999; 11: 17–24.
- 8 Tommasino C, Grana C, Lucignani G, Torri G, Fazio F. Regional cerebral metabolism of glucose in comatose and vegetative state patients. *J Neurosurg Anesthesiol* 1995; **7**: 109–116.
- 9 Gjedde AH, Bauer WR, Wong DF. *Neurokinetics: the dynamics of neurobiology in vivo*. Springer: New York, USA, 2011.
- 10 Shulman RG, Hyder F, Rothman DL. Baseline brain energy supports the state of consciousness. Proc Natl Acad Sci USA 2009; 106:11096–11101
- 11 Hyder F, Fulbright RK, Shulman RG, Rothman DL. Glutamatergic function in the resting awake human brain is supported by uniformly high oxidative energy. J Cereb Blood Flow Metab 2013; 33:339–347
- 12 Demertzi A, Soddu A, Laureys S. Consciousness supporting networks. *Curr Opin Neurobiol* 2013; **23**:239–244
- 13 Dehaene S, Changeux J-P. Experimental and theoretical approaches to conscious processing. *Neuron* 2011; **70**:200–227
- 14 Vanhaudenhuyse A, Noirhomme Q, Tshibanda LJ-F, Bruno M-A, Boveroux P, Schnakers C *et al.* Default network connectivity reflects the level of consciousness in non-communicative brain-damaged patients. *Brain* 2010; **133**:161–171
- 15 Seeley WW, Menon V, Schatzberg AF, Keller J, Glover GH, Kenna H et al. Dissociable intrinsic connectivity networks for salience processing and executive control. J Neurosci 2007; 27:2349–2356
- 16 Vanhaudenhuyse A, Demertzi A, Schabus M, Noirhomme Q, Bredart S, Boly M et al. Two distinct neuronal networks mediate the awareness of environment and of self. J Cogn Neurosci 2011; 23:570–578
- 17 Giacino JT, Fins JJ, Laureys S, Schiff ND. Disorders of consciousness after acquired brain injury: the state of the science. *Nat Rev Neurol* 2014; **10**:99–114
- 18 Thibaut A, Bruno M-A, Chatelle C, Gosseries O, Vanhaudenhuyse A, Demertzi A et al. Metabolic activity in external and internal awareness networks in severely brain-damaged patients. J Rehabil Med 2012; 44:487–494
- 19 Nakase-Richardson R, Yablon SA, Sherer M, Nick TG, Evans CC. Emergence from minimally conscious state: insights from evaluation of posttraumatic confusion. *Neurology* 2009; **73**:1120–1126
- 20 Giacino JT, Kalmar K, Whyte J. The JFK Coma Recovery Scale-Revised: measurement characteristics and diagnostic utility. Arch Phys Med Rehabil 2004; 85:2020–2029
- 21 Seel RT, Sherer M, Whyte J, Katz DI, Giacino JT, Rosenbaum AM *et al.* Assessment scales for disorders of consciousness: evidence-based recommendations for clinical practice and research. *Arch Phys Med Rehabil* 2010; **91**:1795–1813
- 22 Sokoloff L, Reivich M, Kennedy C, Rosiers Des MH, Patlak CS, Pettigrew KD et al. The [14C]deoxyglucose method for the measurement of local cerebral glucose utilization: theory, procedure, and normal values in the conscious and anesthetized albino rat. J Neurochem 1977; 28:897–916
- 23 Takagi S, Takahashi W, Shinohara Y, Yasuda S, Ide M, Shohtsu A et al. Quantitative PET cerebral glucose metabolism estimates using a single non-arterialized venous-blood sample. Ann Nucl Med 2004; 18:297–302
- 24 Strauss LG, Pan L, Cheng C, Dimitrakopoulou-Strauss A. (18)F-Deoxyglucose (FDG) kinetics evaluated by a non-compartment model based on a linear regression function using a computer based simulation: correlation with the parameters of the two-tissue compartment model. Am J Nucl Med Mol Imaging 2012; 2:448–457
- 25 Kuwabara H, Gjedde A. Measurements of glucose phosphorylation with FDG and PET are not reduced by dephosphorylation of FDG-6-phosphate. J Nucl Med 1991; 32:692–698
- 26 Gjedde A. Positron Emission Tomography of Brain Glucose Metabolism with [<sup>18</sup>F] Fluorodeoxyglucose in Humans. In: Hirrlinger J, Waagepetersen H (eds). Brain Energy Metabolism, Neuromethods, Vol 90. Springer Science + Business Media: New York, 2014.

- 27 Darkner S, Sporring J. Locally orderless registration. IEEE Trans Pattern Anal Mach Intell 2013; 35:1437–1450
- 28 Desikan RS, Ségonne F, Fischl B, Quinn BT, Dickerson BC, Blacker D et al. An automated labeling system for subdividing the human cerebral cortex on MRI scans into gyral based regions of interest. *Neuroimage* 2006; 31:968–980
- 29 Sibson NR, Dhankhar A, Mason GF, Rothman DL, Behar KL, Shulman RG. Stoichiometric coupling of brain glucose metabolism and glutamatergic neuronal activity. *Proc Natl Acad Sci USA* 1998; **95**:316–321
- 30 Schlünzen L, Juul N, Hansen KV, Cold GE. Regional cerebral blood flow and glucose metabolism during propofol anaesthesia in healthy subjects studied with positron emission tomography. *Acta Anaesthesiol Scand* 2012; **56**:248–255
- 31 Schlünzen L, Juul N, Hansen KV, Gjedde A, Cold GE. Regional cerebral glucose metabolism during sevoflurane anaesthesia in healthy subjects studied with positron emission tomography. *Acta Anaesthesiol Scand* 2010; 54:603–609
- 32 Alkire MT, Pomfrett CJ, Haier RJ, Gianzero MV, Chan CM, Jacobsen BP et al. Functional brain imaging during anesthesia in humans: effects of halothane on global and regional cerebral glucose metabolism. Anesthesiology 1999; 90:701–709
- 33 Maquet P. Functional neuroimaging of normal human sleep by positron emission tomography. J Sleep Res 2000; 9:207–231
- 34 Kotchoubey B, Merz S, Lang S, Markl A, Müller F, Yu T et al. Global functional connectivity reveals highly significant differences between the vegetative and the minimally conscious state. J Neurol 2013; 260:975–983
- 35 White NS, Alkire MT. Impaired thalamocortical connectivity in humans during general-anesthetic-induced unconsciousness. *Neuroimage* 2003; 19:402–411
- 36 Laureys S, Faymonville ME, Luxen A, Lamy M, Franck G, Maquet P. Restoration of thalamocortical connectivity after recovery from persistent vegetative state. *Lancet* 2000; **355**:1790–1791
- 37 Boly M, Garrido MI, Gosseries O, Bruno M-A, Boveroux P, Schnakers C *et al.* Preserved feedforward but impaired top-down processes in the vegetative state. *Science* 2011; **332**:858–862
- 38 Maandag NJG, Coman D, Sanganahalli BG, Herman P, Smith AJ, Blumenfeld H et al. Energetics of neuronal signaling and fMRI activity. Proc Natl Acad Sci USA 2007; 104:20546–20551
- 39 Goldfine AM, Victor JD, Conte MM, Bardin JC, Schiff ND. Determination of awareness in patients with severe brain injury using EEG power spectral analysis. *Clin Neurophysiol* 2011; **122**:2157–2168
- 40 Lechinger J, Bothe K, Pichler G, Michitsch G, Donis J, Klimesch W et al. CRS-R score in disorders of consciousness is strongly related to spectral EEG at rest. J Neurol 2013; 260:2348–2356
- 41 King J-R, Sitt JD, Faugeras F, Rohaut B, Karoui El I, Cohen L et al. Information sharing in the brain indexes consciousness in noncommunicative patients. *Curr Biol* 2013; 23:1914–1919
- 42 Silva S, Alacoque X, Fourcade O, Samii K, Marque P, Woods R *et al.* Wakefulness and loss of awareness: brain and brainstem interaction in the vegetative state. *Neurology* 2010; **74**:313–320
- 43 Långsjö JW, Alkire MT, Kaskinoro K, Hayama H, Maksimow A, Kaisti KK et al. Returning from oblivion: imaging the neural core of consciousness. J Neurosci 2012; 32:4935–4943
- 44 Vogt BA, Laureys S. Posterior cingulate, precuneal and retrosplenial cortices: cytology and components of the neural network correlates of consciousness. *Prog Brain Res* 2005; **150**:205–217
- 45 Voss HU. Possible axonal regrowth in late recovery from the minimally conscious state. J Clin Invest 2006; **116**:2005–2011
- 46 Fernández-Espejo D, Junque C, Bernabeu M, Roig-Rovira T, Vendrell P, Mercader JM. Reductions of thalamic volume and regional shape changes in the vegetative and the minimally conscious states. J Neurotrauma 2010; 27:1187–1193
- 47 Adams JH, Graham DI, Jennett B. The neuropathology of the vegetative state after an acute brain insult. *Brain* 2000; **123**(Pt 7):1327–1338
- 48 Schiff ND, Giacino JT, Kalmar K, Victor JD, Baker K, Gerber M et al. Behavioural improvements with thalamic stimulation after severe traumatic brain injury. *Nature* 2007; 448:600–603
- 49 Llinás R, Ribary U, Contreras D, Pedroarena C. The neuronal basis for consciousness. *Philos Trans R Soc Lond B Biol Sci* 1998; **353**:1841–1849
- 50 Schiff ND, Ribary U, Moreno DR, Beattie B, Kronberg E, Blasberg R *et al.* Residual cerebral activity and behavioural fragments can remain in the persistently vegetative brain. *Brain* 2002; **125**:1210–1234

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