Acute Clinical and Angiographic Results With the New AVE Micro Coronary Stent in Bailout Management

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To determine the feasibility and safety of deployment of this new stent, we deployed 28 AVE Micro stents in 23 native coronary artery lesions in 20 patients who developed acute or threatened closure after balloon angioplasty (BA). Ten stents were deployed in the left anterior descending artery, 10 in the circumflex, and 8 in the right coronary artery. Luminal dimensions were measured using a computer-based quantitative coronary angiographic analysis system (CAAS II). Stent deployment was successful in 27 of 28 attempts (96%). In 1 patient with a threatened closure of the left anterior descending artery associated with proximal vessel tortuosity, attempted stent deployment was unsuccessful. The clinical course of the other 19 patients in whom stent deployment was successful was free of coronary reintervention, bypass surgery, and death. A myocardial infarction was observed in 2 patients (10%), in 1 of whom the stent was implanted within 24 hours after the onset of acute myocardial infarction, and in the other acute vessel occlusion was present for 58 minutes before stent implantation. No subacute occlusion was observed. Event-free survival at 30 days after stent implantation was 85% (17 of 20 patients). Minimal luminal diameter was 0.85 ± 0.57 mm before and 1.19 ± 0.66 mm after BA, 2.61 ± 0.39 mm during balloon inflation, 3.26 ± 0.46 mm during and 2.74 ± 0.51 mm after stenting, 3.43 ± 0.52 mm during balloon inflation after stenting (Swiss Kiss), and 2.85 ± 0.48 mm after Swiss Kiss. Average percent diameter stenosis was reduced from 69% before through 56% after BA to 17% after stenting. During the initial stent implantation, stent recoil was 0.52 ± 0.30 mm (16 ± 9% of minimal luminal diameter during stent inflation). A Swiss Kiss was performed in 14 stents with an average pressure of 14 ± 4 atm, and residual stenosis was reduced from 2.55 mm (21% diameter stenosis) to 2.85 mm (15% diameter stenosis) in these lesions. Angiographic success (>30% residual diameter stenosis) was achieved in all stented lesions. The results of this early experience would indicate that the new AVE Micro stent may be deployed with a high procedural success rate and a minimal learning curve. Implantation of the stent for the bailout management of failed BA can be achieved with a low incidence of adverse cardiac events and a high angiographic success rate.

METHODS

Patients: To determine the feasibility and safety of deployment of this new stent, we placed 28 AVE Micro stents in 23 native coronary artery lesions in 20 patients who developed acute or threatened closure after BA. The average age was 56 ± 7 years (range 45 to 68), and 17 patients were men. Thirteen patients had stable angina, and the remaining 7 patients had unstable angina. Of the 7 patients with unstable angina, 4 had Braunwald type II and 3 had type III angina. Criteria of acute and threatened vessel closure: After BA, lesion morphology was categorized according to the dissection criteria proposed by Huber et al. and coronary flow distal to the lesion was classified according to the Thrombolysis in Myocardial Infarction trial (TIMI) criteria. Acute occlusion was defined as TIMI 0 flow. Threatened closure was defined as TIMI 1, 2, or 3 flow.
with visible dissection type C, D, E, or F, or as dissection type A or B and TIMI 1, 2, or 3 flow with a residual diameter stenosis of >50%.18,19

**Stent design:** This short stent is characterized by a simple balloon-expandable deployment technique, and 0.008-inch stainless steel struts with moderate radiopacity and a zigzag structure. The metallic surface area in the expanded state has been found in vitro to be 8.4% for the stent with a 3.5 mm diameter. This stent is composed of 4 mm welded and unconnected segments providing a range of lengths from 4 to 16 mm (Figure 1).

**Balloon angioplasty and stent implantation:** BA and stent deployment (Figure 1) were performed according to standard clinical practice by the femoral approach at the Thoraxcenter (Rotterdam, The Netherlands). The coronary stents were delivered on a premounted balloon catheter. The size of the balloon is 0.25 mm larger than the stent diameter to allow for stent recoil. Selection of the nominal stent size was determined to match the vessel reference diameter obtained from on-line quantitative angiographic measurement. Of the 28 stents used in 23 lesions, 9 had a 3 mm diameter, and 15 had a 3.5 mm and 4 a 4 mm diameter. Of the 28 stents 7 were 4 mm in length, 17 were 8 mm, 2 were 12 mm, and 2 were 16 mm. During primary BA, the nominal balloon diameter was 2.98 ± 0.41 mm, and the maximal inflation pressure given was 9.3 ± 3.0 atm. After initial deployment of the stent, high-pressure inflations (14.6 ± 3.5 atm) to optimize stent expansion (Swiss Kiss) were obtained with balloons with 3.50 ± 0.55 mm nominal diameter.

**Anticoagulant therapy:** At the beginning of the procedure, patients were given an intravenous bolus dose of 10,000 IU of heparin, and subsequently 3,000 IU, as required, to maintain the activated clotting time of >300 seconds throughout the procedure. The postintervention anticoagulant regimen was conventional20: One hour after removal of the femoral sheath, a heparin intravenous infusion was begun to maintain the activated partial thromboplastin time between 70 and 90 seconds until oral anticoagulant therapy (warfarin) had achieved a prothrombin time international normalized ratio of 2.5 to 3.5. Warfarin was prescribed for 3 months after stent implantation, and aspirin indefinitely.20

**Quantitative coronary angiographic analysis:** The new version of the CAAS II analysis21,22 was used to perform quantitative analysis. In the CAAS II analysis, which has previously been described elsewhere,52-24 the entire cineframe of 18 × 24 mm is digitized at a resolution of 1,329 × 1,772 pixels. Correction for pincushion distortion is performed before analysis. Boundaries of a selected coronary segment are detected automatically. The absolute diameter (mm) of the stenosis is determined using the guiding catheter as a scaling device. To standardize the method of angiographic analysis, the following measures were taken: All study frames selected for analysis were end-diastolic to minimize motion artifact, and arterial segments were measured between the same identifiable branch points at each stage of the procedure.

**Study end points and definitions:** The primary clinical end point of the study was the occurrence of any of the following adverse cardiac events: acute or subacute stent thrombosis, repeat intervention, coronary artery bypass surgery, myocardial infarction, or death. Procedural success was defined as technically successful deployment of the stent in the absence of an adverse cardiac event. Angiographic success was defined as a <50% residual diameter stenosis after final deployment of the stent. Subacute thrombosis was defined as a stent thrombosis within 14 days of deployment. Acute clinical outcome included all cardiovascular events occurring within 1 month of stent deployment.

**Statistical analysis:** A paired Student’s t test was used to compare sequential changes at the same segment in the same patients. A p value <0.05 was considered significant.

**Figure 1.** An 8 mm AVE Micro stent. The AVE Micro stent is a premounted balloon-expandable stainless steel stent composed of 4 mm welded or unconnected segments.
RESULTS

Lesion characteristics: Angiographic characteristics of the treated lesions are listed in Table I. Of 23 lesions, 8 lesions were in the left anterior descending coronary arteries, 6 were in the right coronary arteries, and the remaining 9 were in the circumflex coronary arteries. Four of the lesions were ostial and 5 were at sites of major bifurcation. Before BA, the lesions were categorized according to the American Heart Association/American College of Cardiology Task Force criteria. Of the 23 lesions, 2 were type A, 15 were type B, and the remaining 6 were type C. After primary BA, at the time of acute or threatened vessel closure, 2 lesions had a type A dissection (with >50% diameter stenosis), 4 a type B dissection (with >50% diameter stenosis), 8 a type C, 1 a type D, 7 a type E, and 1 a type F dissection. At this time, TIMI flow was grade 0 in 1 lesion, grade 2 in 8, and grade 3 in 14 lesions, and the angiographic appearance of intracoronary thrombus (intraluminal filling defect) was present in 7 lesions.

Procedural outcome: Stent delivery was possible in 27 of 28 stents (96%). In 1 patient, the stent could not be advanced beyond an oblique curved branch point to the target stenosis in the midleft anterior descending artery. The unexpanded stent was withdrawn through the guiding catheter without difficulty and the patient was managed by emergency bypass surgery, after which the patient had no further event. In a second patient, a 12 mm stent was deployed at the origin of the left anterior descending artery. During the process of stent inflation, the proximal 4 mm unit of the 12 mm stent migrated proximally into the mainstem of the left coronary artery. This 4 mm unit was then expanded fully in the left mainstem and the patient had an uneventful clinical course.

In-hospital events: One patient in whom stent delivery was unsuccessful underwent emergency bypass surgery and had a normal postoperative recovery. The clinical course of the other 19 patients in whom stent deployment was successful was free of coronary re-intervention, bypass surgery, and death. A myocardial infarction was observed in 2 patients (10%), in 1 of whom the stent was implanted within 24 hours after the onset of acute myocardial infarction, and in the other patient acute vessel occlusion was present for 58 minutes before stent implantation. A femoral hemorrhage and hematuria requiring blood transfusion were observed in 1 patient (5%). All patients remained event free after hospital discharge, and thus the event-free survival at 30 days follow-up was 85% (17 of 20 patients).

Quantitative angiographic analysis: Quantitative angiographic analysis provided measurements of luminal diameter at each procedural phase. Minimal luminal diameter (MLD) was seen to change from $0.85 \pm 0.57 \text{ mm}$ before primary BA to $1.19 \pm 0.66 \text{ mm}$ after BA at the time of dissection. Implantation of the AVE Micro stent increased the MLD to $2.74 \pm 0.51 \text{ mm}$ (p < 0.001). The changes in MLD from before primary BA through stent implantation to after Swiss Kiss are shown in Figure 2. In 14 lesions requiring poststent balloon dilatation (Swiss Kiss), the MLD increased significantly from $2.55 \pm 0.52 \text{ mm}$ (before Swiss Kiss) to $2.85 \pm 0.48 \text{ mm}$ (after Swiss Kiss, p < 0.01). The absolute value of the acute stent recoil in the initial implantation (MLD during stent inflation, MLD after stent) was $0.52 \pm 0.30 \text{ mm}$, and the acute recoil ratio of this stent (MLD during stent inflation, MLD after/during stent inflation) was $16 \pm 9\%$. An example of the stent implantation in the dissection after BA can be seen in Figure 3. Angiographic success was achieved in all lesions with successful deployment of the stent. Thus, the angiographic success rate of all lesions attempted was 96% (22 of 23 lesions). Average percent diameter stenosis decreased significantly from 69% before intervention to a final residual value of 17% after stent deployment. Figure 4 shows the sequential changes in percent diameter stenosis. Performance of a Swiss Kiss in 14 lesions achieved a further reduction in residual percent diameter stenosis from 21% after AVE to 15% after Swiss Kiss (p < 0.05).

DISCUSSION

The key findings of this early experience were as follows: (1) Delivery of the AVE Micro stent to the target lesion can be achieved in a high proportion of cases (22 of 23 lesions). (2) After delivery of the stent (22 lesions), angiographic success as defined by <30% residual diameter stenosis can be achieved in a high proportion of cases (22 of 22). (3) Acute recoil after dilatation of the Micro stent in vivo compares favorably with other stents. (4) Despite the bailout indication for stenting, deployment of the Micro stent resulted in a low risk of acute or subacute stent thrombosis (0 of 22 stented lesions). Successful delivery of the Micro stent may be attributed to 7 characteristics of the stent design. First, the 1.65 mm profile of the Micro stent in its...
unexpanded balloon-mounted state compares favorably with that of previous stents, and thus an intraprocedural exchange of the guiding catheter or guidewire should rarely be necessary. Second, the unconnected junctions of the modules and the 4 and 8 mm length of the individual modules provide the stent with hinge joints and very limited rigid segments to aid the negotiation of tortuous vessels. Furthermore, these 2 features, in conjunction with the primarily longitudinal orientation of the stent struts, should permit passage of an additional Micro stent through a proximally placed stent when necessary. The proximal migration during inflation of a 4 mm segment of an unconnected 12 mm stent into the left mainstem in 1 of our patients, indicates that only connected (welded) units of the AVE Micro stent should be placed in ostial lesions to prevent such an occurrence.

Although 21 of 23 lesions had dissection type B, C, D, E, and F after primary BA, stenting was effective in tacking back the dissection flap and restoring TIMI 3 flow in all lesions stented. Although 7 of the lesions with threatened closure had angiographic evidence of intracoronary thrombus before stenting, deployment of the Micro stent without the administration of intracoronary thrombolytic therapy resulted in neither acute nor subacute thrombosis during follow-up. The absence of stent thrombosis may relate to the low metallic surface area of the Micro stent (8.4% for the 3.5 mm stent in the expanded state) and the optimal expansion of the stent (<30% residual diameter stenosis in all stented lesions), with the additional performance, when necessary, of a Swiss Kiss.

Two of our patients (10%) had significantly elevated creatine phosphokinase levels and electrocardiographic changes in myocardial infarction. In 1 of these 2 patients, stent implantation was performed within 24 hours of the onset of an acute Q-wave myocardial infarction, and the patient became asymptomatic after stenting and creatine phosphokinase levels continued to increase. In the other patient, acute vessel closure had been present for 58 minutes before stent deployment. This patient had no further chest pain after stent implantation and the peak creatine phosphokinase level in this patient was 720 IU/L. Lincoff et al. indicated that peak creatine phosphokinase levels directly related to the time of stent placement after the onset of vessel closure and significant creatine phosphokinase elevation was frequently observed when vessel closure persisted for >49 minutes. Thus, the elevated creatine phosphokinase levels in our 2 patients were believed to reflect their clinical events before stent deployment rather than the occurrence of an acute or subacute thrombosis after stenting.

Both single center and multicenter observational series of bailout stenting have been reported for the Wallstent, Palmaz-Schatz stent, and Gianturco Roubin stent. These have been associated with a deployment success...
rate of 89% to 98%, a myocardial infarction rate of 4% to 43%, a bypass surgery rate 1% to 60%, a subacute thrombosis rate 7% to 16%, and a mortality rate of 1% to 7%. More recently, a number of new stents have become available for clinical evaluation: these include the Cordis and Advanced Cardiovascular Systems stents. Whereas the structural design of these stents can be grouped into 2 categories of mesh stents and coil stents, the AVE Micro stent represents a new design concept. Given their fundamental differences in structural design (profile in the unexpanded state, longitudinal flexibility, mechanism of deployment, metallic surface area in the expanded state, interstir distance, strut orientation, and radial strength), each stent will have to prove its own safety and efficacy for each clinical indication in prospective trials. It is likely that stents with a low metallic surface may be more suited to the more thrombogenic substrate of bailout stenting, while the more rigid mesh stents with higher metallic surface area may be more suited to the elective treatment of primary or recurrent stenoses with strong elastic recoil in nontortuous vessels.

This study revealed considerable changes in luminal diameter from before primary intervention, through stent implantation, to the performance of a Swiss Kiss. Percent diameter stenosis decreased from 69% (before BA) through 56% (after BA) to 15% (after Swiss Kiss). Whereas previous in vitro testing of this stent has found recoil to be 8.7% for the 3.5 mm diameter stent, in this quantitative angiographic study of the stent in diseased coronary arteries in vivo, we found recoil to be 16 ± 9% (0.52 mm), with an average stent diameter of 3.41 mm. Furthermore, the poststent MLD achieved matched or was greater than the nominal stent size in only 3 of 22 stented lesions. The performance of a high-pressure (14 atm) Swiss Kiss may result in an increase in MLD by 0.31 mm, and may be a useful complementary technique when on-line quantitative angiographic analysis is available to guide the optimization of stent deployment.

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