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1 **REALISING THE POTENTIAL OF VARIOUS INHALED AIRWAY CHALLENGE**
2 **AGENTS THROUGH IMPROVED DELIVERY TO THE LUNGS**

3

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9 **Competing interests statement**

10 DS reports grants and personal fees from Almirall, AstraZeneca, Boehringer Ingelheim,

11 Chiesi, GlaxoSmithKline, Glenmark, Johnson and Johnson, Merck, NAPP, Novartis, Pfizer,

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13 outside the submitted work. HWF reports that his employer receives royalties on the sales of

14 the Genuair inhaler from AstraZeneca and royalties on the sales of the Novolizer inhaler from

15 MEDA, outside the submitted work. HWF has a patent PCT/NL2004/000427 licensed to

16 PureIMS, which involves the inhaler technology used for administration of the dry powder

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20 scientific basis. AJL, GWC, CPP and BF declare that they have no competing interests.

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24

1 **Abstract**

2 Inhaled airway challenges provoke bronchoconstriction in susceptible subjects and are a
3 pivotal tool in the diagnosis and monitoring of obstructive lung diseases, both in the clinic
4 and in the development of new respiratory medicines. This article reviews the main challenge
5 agents that are in use today (methacholine, mannitol, adenosine, allergens, endotoxin) and
6 emphasises the importance of controlling how these agents are administered. There is a
7 danger that the optimal value of these challenge agents may not be realised due to suboptimal
8 inhaled delivery; thus considerations for effective and reproducible challenge delivery are
9 provided. This article seeks to increase awareness of the importance of precise delivery of
10 inhaled agents used to challenge the airways for diagnosis and research, and is intended as a
11 stepping stone towards much-needed standardisation and harmonisation in the administration
12 of inhaled airway challenge agents.

13

14

15 **Key words:** bronchial challenge test, bronchial hyperresponsiveness, asthma, drug delivery,
16 delivery method optimization, delivery method standardization

17

1 **1. Introduction**

2 Inhaled airway challenges are a key tool in the study and diagnosis of obstructive lung
3 diseases. Bronchial challenge tests that measure bronchial hyperresponsiveness (BHR) of the
4 airways have established applications in the clinic, where they are used to rule out or confirm
5 a diagnosis of asthma (1,2). Inhaled airway challenges can also be used to study disease
6 mechanisms and symptoms other than BHR, either by varying the outcome measure (e.g.
7 inflammation measured by exhaled nitric oxide or inflammatory cell count) or the stimulus
8 (e.g. allergen or endotoxin). The various airway challenges thereby allow the monitoring of
9 disease activity and effectiveness of treatments (3), and they can provide a robust disease
10 model in early phase clinical trials (4,5). Given the reliance on inhaled airway challenges in
11 respiratory medicine, there is surprisingly little standardisation of techniques or guidance
12 regarding the administration of different test agents. In this article we consider various
13 challenge agents and discuss the importance of standardisation and harmonisation of their
14 administration methods.

15
16 Historically, bronchial challenge tests have been developed to measure BHR by means of
17 spirometry and the change in forced expiratory volume in one second (FEV_1) is still
18 considered the primary outcome measure in the recently published technical standard on
19 methacholine challenge testing (6). However, whether FEV_1 is the most appropriate outcome
20 measure is subject of debate and a recent study points out that the change in effective specific
21 airway conductance (sG_{eff}) measured with body plethysmography actually has a much larger
22 diagnostic value than FEV_1 for the challenge agent methacholine (7). Other techniques that
23 can be used to measure airway function after provocation include forced or impulse
24 oscillometry (airway resistance) (8) and multiple breath nitrogen washout (ventilation
25 heterogeneity) (9). The relative value of these techniques in challenge testing is beyond the

1 scope of this paper. In this review we will refer to the outcome measure in a general way in
2 appreciation of this on-going discussion.

3

4 **2. Inhaled airway challenge agents**

5 Bronchial challenge testing can be performed with a wide range of stimuli, with selection of a
6 particular agent depending on the aim of the test. BHR can be measured using stimuli that
7 have either a direct effect on airway smooth muscle (ASM) (e.g. methacholine or histamine)
8 or an indirect effect where the inhaled agent stimulates inflammatory or neuronal cells (e.g.
9 mannitol, bradykinin or AMP) (10). Furthermore, certain agents can be used that trigger other
10 (patho)physiological mechanisms in the airways (e.g. endotoxin-induced inflammation or
11 allergen-induced responses in allergic subjects), possibly accompanied by BHR in susceptible
12 subjects.

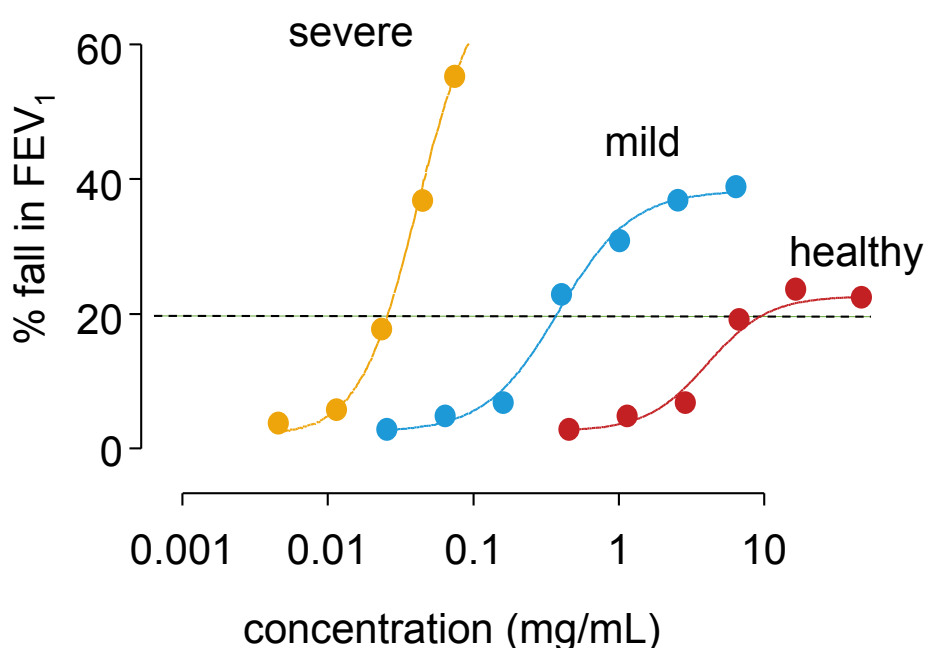
13

14 **2.1 Direct challenge agents**

15 The most commonly used stimulus in bronchial challenge testing is the direct-acting stimulus
16 methacholine, a synthetic analogue of the neurotransmitter acetylcholine that acts as an
17 agonist on muscarinic M₃ receptors on ASM cells. Histamine, an agonist for the histamine H₁
18 receptors on ASM cells, can also be used, although this compound is associated with more
19 systemic side effects such as flushing and headache due to vasodilation (11). When a direct-
20 acting stimulus is used the test generally has a high sensitivity for asthma, meaning that the
21 majority of asthma patients will respond to this stimulus, and the responsiveness increases
22 with the severity of lung disease (1). However, the specificity is poor since healthy subjects
23 also respond when the dose is high enough; they are just less sensitive and less reactive to the
24 stimulus than asthmatic subjects (**Figure 1**). Even though cut-off values for healthy and
25 hyperresponsive individuals have been agreed upon (1,6,11), these values can still be

1 considered as quite arbitrary due to the many factors affecting lung deposition of the stimulus,
2 such as the patient's breathing pattern or the presence of emphysema, inflammation, mucus
3 deposition and/or oedema. Moreover, it is becoming clear that methacholine can miss newly
4 diagnosed asthmatic subjects whose symptoms are mild and whose lung function is excellent,
5 but who demonstrate asthma in terms of significant exercise-induced bronchoconstriction
6 (12). However, the use of a different predefined threshold value for the outcome measure in
7 methacholine challenge as compared to exercise-induced bronchoconstriction (*i.e.*, 20%
8 reduction in FEV₁ in the former versus 10–15% reduction in FEV₁ in the latter) may explain,
9 at least in part, such discrepancy. Additionally, testing with methacholine does not allow for
10 absolute differentiation between patients with asthma or COPD, or indeed other diseases such
11 as allergic rhinitis (13–16).

12



13

14 **Figure 1: Dose-response curves to inhaled methacholine in a healthy, mild-asthmatic, and**
15 **severe-asthmatic subject, showing both the leftward shift of the curve (hypersensitivity) and**
16 **steeper slope (hyperreactivity) that characterise BHR. Reproduced with permission from the**
17 **European Respiratory Society (1,117).**

1 **2.2 Indirect challenge agents**

2 In the search for stimuli that produce responses through mechanisms that better reflect the
3 underlying disease pathology, indirect challenges have been introduced, which exert their
4 effects on intermediary cells involved in the asthmatic response, rather than acting directly on
5 ASM. Most indirect stimuli evoke a heterogeneous response by affecting multiple
6 pathophysiological pathways (3). Especially in the 1980s and 1990s many different potential
7 indirect stimuli have been investigated, which have been reviewed comprehensively by Van
8 Schoor et al., first in 2000 (10), and subsequently updated in 2005 by the same authors (17).
9 In 2003, a European Respiratory Society (ERS) Task Force published their recommendations
10 on the use of indirect stimuli in diagnosis and monitoring of asthma (3).

11

12 Indirect stimuli can be sub-classified as physical or pharmacological stimuli. Physical stimuli
13 induce airways obstruction without acting on specific receptors, exemplified by exercise-
14 induced bronchoconstriction or that induced by “fog” challenges with distilled water or
15 hypotonic aerosols (18,19). Exercise induces dehydration of the airway epithelium, resulting
16 in an increased osmolarity of the airway lumen and subsequent release of mediators from
17 mast cells and activation of sensory nerves (20). This process is mimicked during challenge
18 with hyperosmolar aerosols (21,22). Pharmacological stimuli induce airways obstruction
19 secondary to the activation of intermediary cell types, such as inflammatory, epithelial, or
20 neuronal cells, or combinations of these. The effects of indirect agents depend on the specific
21 cells and receptors involved (10), but many of the stimuli used are known to activate sensory
22 nerves, for example bradykinin, sulphur dioxide and adenosine (reviewed in (23)). Some
23 indirect stimuli are endogenous compounds known to be released during airways obstruction,
24 such as adenosine, AMP, tachykinins and bradykinin (24–31). Another group of indirect-
25 acting stimuli is comprised of sulphur-containing compounds, which originated from the

1 observation that sulphur dioxide, a common air pollutant, and sulphites used as preservatives
2 in food processing, may induce bronchoconstriction in susceptible subjects through activation
3 of sensory neuronal pathways (32,33). However, lack of reproducible test outcomes has led to
4 discontinuation of studying several of these stimuli (sulphur dioxide, sodium metabisulphite,
5 bradykinin and tachykinins) and focus has predominantly shifted to the most easily and
6 widely applicable indirect stimuli, mannitol (physical) and AMP/adenosine
7 (pharmacological).

8

9 **2.3 Allergen challenge**

10 The preceding “non-specific” bronchial challenge tests are targeted to mechanisms that are
11 thought to be intrinsic to the underlying hyperresponsive state of the airways in subjects with
12 asthma. In contrast, so-called “specific” airway challenges can be used to assess the airway
13 responsiveness to sensitising agents, such as aeroallergens or occupational agents. In allergic
14 subjects, following sensitisation to an allergen, minute quantities of that allergen are sufficient
15 to cause an immediate IgE-mediated early asthmatic response (EAR). In approximately 50%
16 of positive allergen challenges a recurrence of airflow obstruction occurs between 3 to 8 hours
17 after allergen exposure, the so-called late asthmatic response (LAR) (34), which is associated
18 with airway inflammation and in some patients can be associated with an increase in BHR to
19 agents like methacholine (35–37). Often-used outcome measures for inhaled allergen
20 challenge are a >15% decrease in FEV₁, >50% decrease in specific airway conductance, or
21 >100% increase in specific airway resistance compared to baseline (38). Additional outcome
22 measures can be the change in non-specific BHR to e.g. methacholine, or the occurrence of
23 airway inflammation expressed as increase in sputum eosinophils or exhaled nitric oxide (38).
24 Inhaled allergen challenge has also been widely used as a model to assess the efficacy of
25 novel therapeutic interventions (39–49).

1 **2.4 LPS challenge**

2 Another interesting application of the inhaled airway challenge test concept is provocation
3 with lipopolysaccharide (LPS), also called endotoxin, a major component of the outer
4 membrane of Gram-negative bacteria that induces fever and inflammation upon systemic
5 exposure (50). Aerosolised endotoxins are present ubiquitously in the environment in
6 concentrations that do not elicit immune responses. However, in certain aerosols, like tobacco
7 smoke and organic dusts, concentrations can be high enough to induce responses in the lungs
8 (51). Inhalation of endotoxin has been associated with lung inflammation, most notably
9 neutrophilia (52–54). It can further lead to bronchial obstruction in people with asthma or
10 other forms of BHR (55,56). Interestingly, it has recently been reported that LPS can elicit
11 BHR through a mechanism involving cholinergic transmission (57).

12
13 Airway challenge with a nebulised LPS solution has been used mainly to study neutrophilic
14 inflammatory processes in the lungs and has been developed into a challenge model to
15 investigate the effect of novel anti-inflammatory drugs under development for the treatment
16 of diseases that are associated with neutrophil infiltration into the lungs, particularly COPD
17 and severe asthma, as this challenge is not sensitive to treatment with glucocorticosteroids
18 (5,58–61). This model has also been used for early proof-of-concept and dose-ranging studies
19 for novel drugs for the treatment of respiratory diseases in healthy volunteers (58,62).

21 **3. General considerations for challenge delivery to the lungs**

22 Despite the wide array of challenge test agents, there are relatively few methods used for their
23 administration. Hence various aspects need to be considered that apply to airway challenge
24 methodology in general, irrespective of the agent that is used.

25

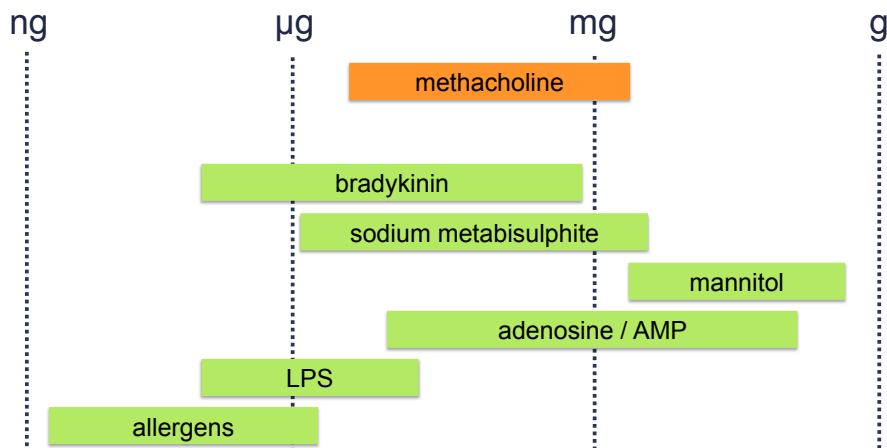
1 3.1 Delivered dose

2 Inhaling a challenge agent usually leads to a dose-dependent response in the lungs. For
3 challenges that induce BHR, the minimal dose required to obtain a response, as well as the
4 slope of the dose-response curve, varies amongst patients and defines the severity of their
5 BHR (1). The aim of such bronchial challenge tests is to induce a pre-defined degree of
6 bronchoconstriction without risking a response that is too severe, meaning that the dose of the
7 stimulus requires titration. For this reason, ascending dosing protocols have been developed
8 in which the stimulus is administered by nebulisation of ascending (usually doubling)
9 concentrations or doses, after each of which the lung function is measured (1,6,11,63,64). The
10 concentration or dose is gradually increased and the test continues until a predefined threshold
11 value for the outcome measure is obtained. The test result is negative when the threshold
12 value is not reached after administration of the top dose.

13
14 This methodology has been initially developed for direct stimuli (65), but indirect-acting
15 stimuli are generally administered following similar dosing protocols (3), although different
16 concentrations (or doses) may be used to accommodate differences in potency, as shown in
17 **Figure 2**. For AMP for example, a 16-fold lower potency has been reported compared to
18 methacholine (66). Allergen exposure should be increased gradually either by extending the
19 duration of the exposure or increasing the concentration in order to prevent severe acute
20 reaction (38). For the same safety reason, allergen dose increments should have longer time
21 intervals (10–15 min) compared to direct or indirect challenge methods (<5 min). Due to their
22 specific mode of action, as little as a few ng can suffice to elicit the airway response.
23 Endotoxin challenge on the other hand is usually administered by nebulisation of a fixed dose
24 in the µg-range.

25

1 It is clear that due to these differences in dosimetry, the various challenges require different
2 methods for administration. However, currently no universally standardised methodology is
3 used in the majority of cases to deliver these different agents. It is important to realise that
4 this may have important implications that are now largely neglected by the field.
5



6
7 **Figure 2: Dose ranges of various inhaled airway challenge agents. Allergens and LPS can also be**
8 **expressed in biological units and endotoxin units respectively.**

10 3.2 Administration by nebulisation

11 Most challenge agents are administered by nebulisation, except for mannitol and an
12 investigational formulation of adenosine that are both administered as a dry powder (see
13 below). Preparing nebuliser formulations can be very straightforward, which is the main
14 reason why nebulisers are often used for off-label or investigational drugs and non-medicinal
15 compounds, like many of the agents used for challenge testing. However, it has to be
16 carefully evaluated whether the formulation affects nebuliser performance (in terms of droplet
17 size and output rate) and, in the case of more complex molecules, whether the nebulisation
18 process leads to degradation of the agent (e.g. allergens of biological origin).

1 Two standardised dosing protocols have been published for administration of methacholine
2 by nebulisation (6,11). The two methods have different pros and cons, and the choice of
3 method has been left to the preference of individual investigators/clinicians. The dosimeter
4 method involves five deep and slow inhalations, which allows for accurate quantification of
5 the administered dose, thereby making this method suitable for studies that require
6 administration of an exact dose, such as LPS challenge studies or allergen challenges using a
7 bolus dose. It has been claimed, however, that such deep breaths have bronchoprotective and
8 bronchodilatory effects per se (67–69), which may therefore interfere with an accurate
9 interpretation of the test result. In the newest technical standard on methacholine challenge
10 testing a deep-breath method is therefore not recommended (6). The other method is the tidal
11 breathing method in which the stimulus is inhaled during a specified time of calm, tidal
12 breathing, although the patient's inhalation flow rate is generally not controlled. This more
13 shallow way of inhaling does not evoke bronchoprotective and bronchodilatory mechanisms,
14 but could result in different deposition patterns of the aerosolised challenge compared to the
15 five-breath dosimeter method, since penetration of the aerosol into the more distal airways is
16 dependent on the mixing of old and new air in the lungs. Moreover, the total amount that is
17 inhaled depends on the inspiratory cycle of the subject, but also on the output rate of the
18 nebuliser. In the first universal (American Thoracic Society) guidelines on methacholine
19 challenge testing, the output rate had therefore been standardised at 0.13 mL/min (based on
20 the output rate of the Wright nebuliser that was commonly used for challenge testing),
21 regardless of the nebuliser that was used (11). However, adjusting the jet pressure to obtain
22 this output rate may have detrimental effects on the droplet size distribution. As an example,
23 this has been shown for the SideStream nebuliser (Philips Respironics), where the median
24 mass aerodynamic diameter (MMAD) increased from 5.1 μm to 8.5 μm when the jet pressure
25 was reduced from 1.5 bar (manufacturer's specifications) to 0.5 bar to reach the required

1 output rate of 0.13 mL/min (70). To prevent such unforeseen changes, a better strategy is to
2 control the total administered volume of the solution containing the challenge agent by
3 altering the nebulisation time rather than using an output rate of the nebuliser outside of the
4 manufacturer's specifications, which is now discussed in the recently published European
5 Respiratory Society technical standard on methacholine challenge testing (6).

6
7 In addition to the effect of jet pressure on droplet size, the type of compound and its
8 concentration may affect the droplet size distribution as well. For AMP, which has a dose
9 range exceeding that of methacholine, it has been shown that the increased viscosity of the
10 more concentrated solutions resulted in a large shift in the aerosol droplet size distribution
11 (70). In this study, a decrease in MMAD of almost 50% was measured at the highest AMP
12 concentration (320 mg/mL) compared to saline and the lowest AMP concentrations. These
13 results indicate that applying methods developed for a certain stimulus and a certain device
14 cannot simply be used for other compounds or in other situations without verifying their
15 suitability.

16
17 A third factor that should be accounted for is the evaporation of solvent (water) during
18 nebulisation. The driving force for evaporation is saturation of the outgoing air with solvent
19 (71), which leads to an increase in concentration of the remainder of the solution in the
20 nebuliser cup (70,72). Importantly, evaporative water losses lead to an overestimation of the
21 administered dose when the output rate is measured gravimetrically (6). Evaporation is an
22 endothermic effect and the energy needed for this process is drawn from the solution,
23 resulting in a temperature drop in the nebuliser solution that in turn may affect the output rate
24 of the nebuliser (72). Calibration of the nebuliser output rate should therefore be performed
25 under precise operating conditions. Newer jet nebulisers and especially vibrating mesh

1 nebulisers exhibit much lower amounts of evaporative loss (6), but still it is preferable to
2 measure output rate by means of filter measurements (collection of the active compound)
3 rather than gravimetrically. Such data should either be provided by the manufacturer or can be
4 obtained in a pharmaceutical lab specialised in inhaled drug delivery.

5

6 In contrast to methacholine, there are no universal standardised protocols for other challenge
7 agents, although recommendations have been made for similar ascending administration
8 protocols (3).

9

10 **3.3 Aerosol deposition and distribution in the lungs**

11 For optimal efficacy and discriminatory power, inhaled medical aerosols should achieve
12 maximal delivery to, and deposition in the target area in the lungs. Bronchial challenges that
13 measure bronchoconstriction should be targeted to the proximal part of the bronchial tree,
14 where the effects of ASM contraction are most pronounced. This means that the requirements
15 for aerosol particle size are quite easily met, since an MMAD of roughly 3 to 5 μm should
16 generally suffice, especially at tidal breathing. Aerosols with particles in this size range have
17 the additional benefit of increased deposition efficacy, resulting in a higher total lung dose
18 compared to particles smaller than 1.5 μm (73). It has indeed been found that aerosols with
19 MMADs of 3 and 5 μm result in a lower methacholine PC_{20} compared to those with an
20 MMAD of 1 μm (74), which can be attributed to a combination of greater lung deposited dose
21 and targeting to the proximal airways.

22

23 It could be reasoned that challenges that act on inflammatory processes should be targeted
24 more distally, as inflammation occurs throughout the lungs. However, investigations into the
25 effects of particle (droplet) size on airway responsiveness to AMP have thus far been

1 inconclusive due to a high number of non-responders to small-particle AMP, which could be
2 explained by a higher exhaled fraction or the discrepancy between deposition in the peripheral
3 airways and an outcome measure of the more central airways (FEV₁) (75). For allergens,
4 significant effects of particle size on the response to cat and mite allergen have been found,
5 with larger particles (around 10 µm) being more effective in inducing the immediate response
6 (76,77). A study investigating the effect of particle size on responses to endotoxin found a
7 greater inflammatory response at the bronchial and systemic level when challenged with
8 larger particles, although it could not be concluded whether this was due to regional
9 distribution differences or the higher total lung dose (78).

10

11 **3.4 Patient-related factors affecting aerosol deposition**

12 Patient-related factors, such as the size and morphology of the oropharynx and bronchial tree,
13 and the severity of lung disease can also affect aerosol deposition patterns (79). Additionally,
14 inhalation flow rate has an important influence on the site of deposition (80). A higher flow
15 rate shifts deposition to the higher airways at the cost of peripheral deposition. The patient's
16 flow rate should therefore be adjusted to the type of delivery device being used to prevent loss
17 of aerosol through deposition in the throat. Newer delivery systems that provide electronic
18 control over the inhalation flow rate and volume (e.g. APS Pro system, see section 4.1, and
19 AKITA) can provide better control over the delivered dose and deposition in the lungs (81–
20 83).

21

22 Current medication use of patients undergoing a bronchial challenge has to be accounted for
23 as well, since these treatments are intended to reduce or prevent the symptoms evoked during
24 the challenge. To prevent possible confounding effects on the test outcome, lung medications
25 have to be withheld for a specified time prior to execution of the test. The duration of

1 withholding is dependent on the mechanism of action of the drug and ranges from a few hours
2 for short-acting beta-agonists up to a few days for long-acting anticholinergics or even weeks
3 for ICS (depending on the challenge agent and the aim of the challenge test).

4

5 **4. Optimisation and standardisation of challenge delivery per agent**

6 Both optimisation and standardisation of challenge methods by different agents are urgently
7 needed, in order to address the issues identified in the preceding section and make scientific
8 progress towards more precise and rigorously controlled diagnostic procedures. Some efforts
9 have already been undertaken in this regard, for example with the mannitol test
10 (Aridol/Osmohale; see section 4.2).

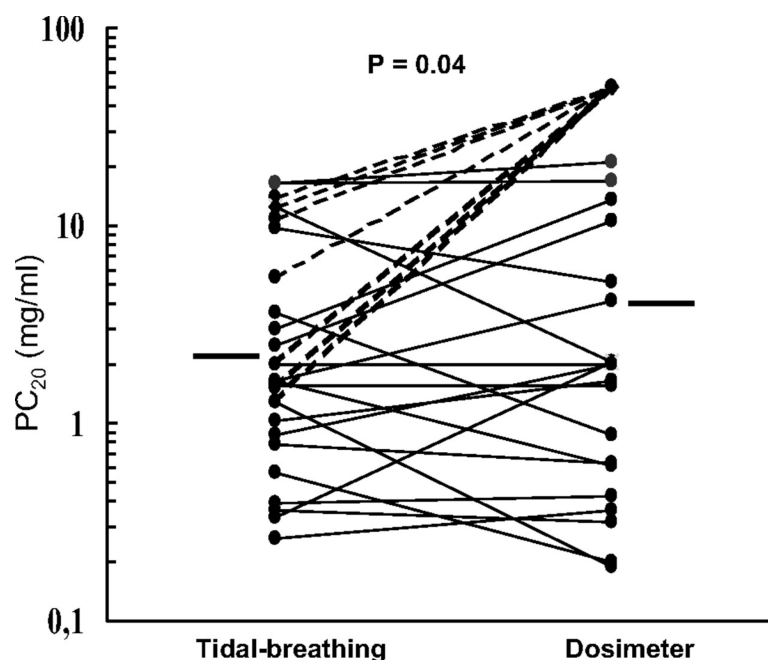
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12 **4.1 Methacholine**

13 Soon after publication of the first universal guidelines for methacholine challenge in 2000,
14 which recommend both the dosimeter method and tidal breathing method, studies began to
15 appear that investigated the comparability of the two dosing protocols. The first study
16 reported similar results (geometric mean PC₂₀ 1.8 mg/mL for tidal breathing vs. 1.6 mg/mL
17 for dosimeter). However, the authors compared different dosing protocols (twofold vs.
18 fourfold increases in concentration for tidal breathing and dosimeter respectively) (84).
19 Cockcroft et al. addressed this disparity by comparing identical dosing regimens (doubling
20 concentrations) and found that the tidal breathing method, which exposes the subject to twice
21 as much aerosol at each concentration, resulted in a PC₂₀ that was 1.6 (PC₂₀ <1 mg/mL) to
22 2.1-fold (PC₂₀ >1 mg/mL) lower compared to the dosimeter method (85). This difference
23 between subjects with mild and severe hyperresponsiveness has been suggested to be
24 explained by bronchodilator and/or bronchoprotective effects of the inhalation manoeuvre
25 adopted in the dosimeter method (85,86). Prieto et al. reported a difference of 0.78 doubling

1 concentrations, with dosimeter values being higher than tidal breathing values, but found
2 similar values for slope and level of plateau of the dose-response curve (87). Acknowledging
3 the difference in administered volume, they performed another study in which they
4 administered the same volume of challenge. Still an average difference in PC_{20} of 0.9
5 doubling concentrations was reported (88). However, when looking at the individual subjects
6 it can be seen that this difference was mainly caused by a higher number of non-responders
7 when using the dosimeter method (**Figure 3**). This may actually indicate that in some subjects
8 with (mild) asthma the bronchodilatory effect of deep inhalations can indeed effectively
9 counteract any bronchoconstriction induced by methacholine, as suggested by Cockcroft et al.
10 (85). Indeed deep-breath methods have now been excluded from the new technical standard
11 on methacholine challenge for this reason (6).

12
13



14

15 **Figure 3: Comparison of tidal breathing and dosimeter methacholine PC_{20} in 27 subjects with**
16 **suspected asthma. The dashed lines indicate seven subjects in whom no dosimeter PC_{20} was**
17 **obtained. Reproduced with permission from (82).**

1 More recent investigations into methacholine challenge method optimisation focused on the
2 delivery systems used, as the nebulisers recommended in the first guidelines (11) had become
3 obsolete (89). The Aerosol Provocation System (APS) Pro (CareFusion) is especially
4 noteworthy in this respect. The APS Pro system is a computer-controlled nebuliser system
5 specifically developed for bronchial challenge testing with methacholine and can be
6 integrated with other CareFusion systems for spirometry, impulse oscillometry, respiratory
7 resistance and body plethysmography depending on the outcome measure of choice. The
8 dosimeter method is the preferred method, although the system can also be used for the tidal
9 breathing method. The PD₂₀ from a pulse of aerosol of a single methacholine concentration
10 was found to correlate well with the PC₂₀ obtained with a standard dosimeter test (90). *In*
11 *vitro* studies indicate that these new delivery systems often have a higher output rate than the
12 systems recommended in the first guidelines, thus a faster delivery of the challenge, which
13 should be controlled for in terms of exposure time (70,89).

14

15 The plethora of available nebuliser systems (with variable output rates) introduces new
16 concerns regarding equivalence of the test results obtained with different systems.
17 Interestingly, it has been found that no differences between test systems are found when the
18 PD₂₀ is calculated (91,92) instead of the PC₂₀ (91,93), which has led to the recommendation
19 to use the PD₂₀ as the end-point in the new technical standard (6). On a different note, using
20 more efficient nebulisers also introduces a risk of extreme individual responses to
21 methacholine aerosols. Patients who are highly responsive to methacholine may experience
22 large drops in FEV₁ when the full dose is presented to them in a shorter time, which should be
23 accounted for by thorough safety assessment of using these more efficient nebulisers.

24

25

1 **4.2 Mannitol**

2 Bronchial challenge with mannitol has been developed to overcome technical difficulties (i.e.
3 the need for filters and scales to determine the administered volume) encountered with
4 bronchial challenge tests using hypertonic saline (20,94,95). This agent has been shown to
5 cause contraction of ASM through release of inflammatory mediators such as leukotriene E₄
6 and prostaglandin D₂, which are thought to be released from mast cells (96). BHR measured
7 in response to inhaled mannitol is dependent on the presence of inflammation and can be
8 reduced by ICS treatment (97,98). The low sensitivity (59.8%) of the mannitol test compared
9 with the clinical assessment determined in more than 500 subjects was attributed to ICS use
10 by 75% of the diagnosed asthmatics in this study, as this value greatly improved when ICS-
11 users were excluded from analysis (to 88.7%) (95). This finding supports the concept that
12 mannitol responsiveness can be used to monitor ICS effectiveness (97,98) and highlights the
13 growing appreciation that indirect challenge tests are useful for diagnosis and monitoring
14 treatment of current asthma. Mannitol responsiveness – expressed as the provocative dose that
15 causes a 15% decrease in FEV₁ (PD₁₅) – has been found to correlate well with responsiveness
16 to bronchial challenge tests with other physical stimuli or AMP (99,100). Bronchial challenge
17 testing with mannitol may therefore be of particular use in diagnosis of asthma in elite
18 athletes, who require an official diagnosis of asthma, but whose bronchoconstriction is hard to
19 induce by exercise in a laboratory setting (101).

20

21 The mannitol challenge test is registered with various regulatory authorities worldwide and is
22 currently the only fully standardised challenge method. The mannitol formulation consists of
23 a spray-dried powder with an MMAD of around 3.5 µm that is inhaled with a simple capsule
24 inhaler device. Benefits of this mannitol test are that it comes in a standardised kit that does
25 not need any special equipment, and that it is relatively easy to perform. However, a

1 drawback of mannitol challenge is the deep inhalation-dependent modality of powder
2 administration, which has been suggested to counteract bronchoconstriction as discussed in
3 section 4.1. Moreover, the quantity of powder that needs to be inhaled is large in comparison
4 to other agents, up to a cumulative dose of 635 mg, as a consequence of its mechanism of
5 action (i.e. increasing the osmolarity of the lung lining fluid). This in combination with the
6 low resistance device, and hence a high inspiratory flow rate, can result in cough through a
7 mechanical cough reflex due to oropharyngeal deposition of the mannitol (102). In a phase III
8 study investigating the safety and efficacy of inhaled mannitol as a bronchial challenge test,
9 cough occurred in 535 of 592 (of whom 91 were non-asthmatic) subjects. In some cases,
10 cough was so severe that the test had to be delayed (one in seven subjects), or even ended
11 prematurely (one in 100 subjects) (95). Although cough does not occur exclusively in subjects
12 with asthma, it has been demonstrated that cough in response to inhaled mannitol is
13 associated with asthma (103), which would be interesting to elucidate further. To which
14 extent the occurrence of (severe) cough is diagnostic for asthma and to which extent it is due
15 to oropharyngeal deposition of mannitol could be investigated by provoking subjects with the
16 same mannitol formulation, but using a high-resistance inhaler device and controlled slow
17 inhalation to minimise throat deposition.

18

19 **4.3 Adenosine**

20 Other efforts towards optimisation have been undertaken with inhaled adenosine. Adenosine
21 and its precursor AMP have been the subject of a considerable amount of research in
22 respiratory medicine since the early 1980s. Adenosine, a purine nucleoside involved in many
23 biological processes, is considered a pro-inflammatory mediator in asthma (104) as it is
24 thought to induce mast cell degranulation, a process mediated through the A_{2b} receptor,
25 leading to contraction of ASM and most notably airway eosinophilia (105,106). More

1 recently a role for A₁ receptors has been implicated in the contraction of ASM from subjects
2 with asthma induced by adenosine (107), suggesting that adenosine triggers
3 bronchoconstriction through both inflammatory and neuronal pathways.
4
5 Historically, AMP has been used instead of adenosine because of its much higher aqueous
6 solubility, which is required for nebulisation, and it is generally assumed that AMP is
7 converted in vivo to adenosine instantaneously by endonucleotidases when it comes in
8 contact with lung lining fluid (10). However, because of the above mentioned effects of high
9 AMP concentrations on aerosol particle size produced by nebulisation (70), an adenosine dry
10 powder challenge test has been developed that consists of simple spray-dried formulations
11 containing pure adenosine or adenosine diluted with lactose, which so far have only been
12 administered with an investigational inhaler device. With this inhaler, the entire dose range of
13 adenosine (0.04–80 mg) was consistently delivered in the first proof-of-concept studies that
14 have been performed with this formulation (108–110). So far, these studies justify the chosen
15 dose range for adenosine and indicate that the response rate and thus diagnosis of asthma can
16 be improved by the administration of the higher doses that are possible with the powder
17 formulation. These findings now have to be complemented by studies in healthy subjects and
18 in subjects with lung diseases other than asthma to determine the specificity and sensitivity of
19 this test. Since the test concerns a powder for inhalation, any effects on bronchoconstriction
20 of the deep-inhalation dependent administration should also be considered for this adenosine
21 challenge test.

22

23 **4.4 Occupational agents and allergens**

24 For occupational agents, the suspected causative agent should be delivered in the same
25 conditions that it is found in the workplace in terms of physical and chemical properties in

1 relevant concentrations (38). It is now recognised that there are a large variety of occupational
2 agents and allergens and therefore a handbook has recently been prepared that summarises the
3 delivery methods for the most commonly used agents (see online supplement to (38)). This
4 handbook provides an excellent start towards harmonisation of specific inhaled challenges,
5 although it could benefit from inclusion of recommendations on nebulisers for those agents
6 that are administered following a tidal breathing or dosimeter method.

7
8 Allergens are administered in very low doses compared to the nonspecific bronchial
9 challenges. Nebulisation can therefore in general be considered a suitable administration
10 method, provided the stability of the agent is checked during storage and upon administration,
11 particularly for more complex molecules (e.g. antigens). Chemical stability issues upon
12 storage arise when an agent is sensitive to degradation reactions (e.g. oxidation, hydrolysis),
13 as these occur faster in aqueous conditions than in the dry state. Additionally, stability can
14 become an issue when the stresses induced by the nebulisation process itself may damage the
15 material(s) (e.g. proteins) in the formulation (111,112).

16

17 **4.5 LPS**

18 LPS is very stable and can withstand high temperatures and strong shear forces. It can be kept
19 in solution for up to a month. However, LPS adheres readily and strongly to surfaces such as
20 glass, for example to the vial in which it is stored. Extra care (e.g. rigorous vortexing) should
21 therefore be taken in the preparation of the nebuliser solution. Additionally, endotoxins from
22 different sources can have a different biological activity (potency). Studies report the use of
23 different sources of LPS and different doses, ranging from 0.5 to 100 µg (5,52–54,59–62).
24 However, expressing dose in units of weight has little value because of the different
25 potencies. Variability in the dose delivered to patients is further increased by differences in

1 administration method. Both dosimeter and tidal breathing methods have been used to date
2 and the differences between devices and inhalation manoeuvres inevitably result in
3 differences in the delivered and deposited doses.

4
5 The lack of control of dose in terms of potency, in addition to differences in administration
6 methods, complicates the comparison of studies performed over a period of about 30 years.
7 Studies have been performed in healthy (5,51–54,58–62,113) and diseased subjects
8 (55,56,114,115), in smokers (116) and non-smokers, but the potency of the LPS was often not
9 reported. Although a promising disease model, standardisation of the dosing protocol and
10 administration method should be established before LPS challenge can be accepted as a
11 validated tool to be used more widely in drug development studies. Other issues that need to
12 be addressed are the lack of dose-response studies performed in humans and uncertainty
13 regarding why some people do not respond to LPS inhalation. To study the latter issues, it is
14 imperative to know the exact dose of LPS that is delivered and its potency. The first steps
15 forward should be to decide on a preferred administration method (i.e. slow deep inhalation)
16 and performing a potency measurement of the LPS in the nebuliser solution to be used for
17 administration.

18

19 **5. Conclusions**

20 Inhaled airway challenges are versatile tests that are relatively easy and cheap to perform.
21 Classical bronchial challenge tests that assess BHR have proven their value in excluding or
22 confirming a suspected diagnosis of asthma and have been shown to be useful for monitoring
23 the disease and effectiveness of therapy. These tests can thus help in providing more accurate
24 information to patient and prescriber as to how to treat an individual patient. As such,
25 bronchial challenge tests can help in improving the individual patient's health through better

1 treatment of their disease. In research and development, inhaled airway challenge can be
2 applied even more widely, from studying disease mechanisms to investigating the
3 effectiveness of new drugs. Careful selection of the challenge agent may provide significant
4 benefits, in terms of both selecting suitable subjects (e.g. using response to a discriminatory
5 challenge as an inclusion criterion) and addressing the research question. There is also a lot to
6 be gained through optimisation and reporting of challenge test posology, especially to ensure
7 the comparability of studies performed by different laboratories. In general all compounds
8 described so far would strongly benefit from the development of defined inhalation systems
9 that provide a reproducible and reliable deposition in the lungs and further standardisation of
10 administration protocols as has been done for mannitol (**Table 1**). Improved delivery may
11 also open doors for revisiting some challenge agents that have been used in the past, but were
12 abandoned due to lack of reproducibility. Creating a “tool box” of well-characterised
13 challenge agents with tailored delivery systems would provide a valuable tool for studying
14 and discriminating different airway diseases, but also for investigating mechanisms and novel
15 treatments for affecting BHR.

16

17

1 **Table 1: Opportunities to improve the application of bronchial challenge testing**

Issue	Need
Delivery method optimisation	Control (and quantification) of delivered dose by optimising the production and administration of challenge agent aerosols with suitable aerodynamic size distributions. This will require the tailoring of delivery methods for each individual challenge agent.
Standardisation	International consensus on best practice. Inter-lab comparisons to verify the reproducibility of standard methods. Reporting of dose characterisation/validation for all research studies.
Specific issues for mannitol	Investigate the relative contributions of throat deposition and increased airway sensitivity to the occurrence of cough in asthma.
Specific issues for adenosine	Compare responsiveness to dry powder adenosine challenge to responsiveness to nebulised AMP including the response of healthy subjects and patients with lung diseases other than asthma. Determination of the specificity and sensitivity of dry powder adenosine bronchial challenge in patients with asthma.
Specific issues for allergens	Extension of existing guidelines (37) to include recommendations on nebulisers for those agents that are administered following a tidal breathing or dosimeter method. Verification of chemical stability and tolerance to nebulisation on a case-by-case basis.
Specific issues for LPS	Control of test agent potency and reproducibility of delivery (dose and lung distribution).

2

3

4

5

6

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