



## Glucagon-like Peptide 1 Conjugated to Recombinant Human Serum Albumin Variants with Modified Neonatal Fc Receptor Binding Properties. Impact on Molecular Structure and Half-Life

**Bukrinski, Jens T.; Sønderby, Pernille; Antunes, Filipa; Andersen, Birgitte; Schmidt, Esben G. W.; Peters, Güenther H. J.; Harris, Pernille**

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Article

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Jens Thostrup Bukrinski, Pernille Sønderby, Filipa Antunes, Birgitte Andersen, Esben Gjerloff Wedebye Schmidt, Guenther H. H. J. Peters, and Pernille Harris

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# GLP-1 conjugated to rHSA variants with modified FcRn binding properties. Impact on molecular structure and half-life

Jens T. Bukrinski<sup>2</sup>, Pernille Sønderby<sup>1</sup>, Filipa Antunes<sup>3</sup>, Birgitte Andersen<sup>2</sup>, Esben G. W. Schmidt<sup>2</sup>, Günther H.J. Peters<sup>1</sup>, Pernille Harris<sup>1\*</sup>

<sup>1</sup>Department of Chemistry, Technical University of Denmark, Kemitorvet 207, DK-2800 Kgs. Lyngby, Denmark

<sup>2</sup>Novozymes A/S, Krogshøjvej 36, Bagsværd, DK-2880, Denmark

<sup>3</sup>Albumedix Ltd, Castle Court, 59 Castle Boulevard, Nottingham, NG7 1FD, United Kingdom

E-mail: \*ph@kemi.dtu.dk

## ABSTRACT

Glucagon-like peptide 1 (GLP-1) is a small incretin hormone stimulated by food intake, resulting in an amplification of the insulin response. Though interesting as a drug candidate for the treatment of type 2 diabetes mellitus, its short plasma half-life of less than 3 minutes limits its clinical use. A strategy to extend the half-life of GLP-1 utilizes the long half-life of *human* serum albumin (HSA) by combining the two via chemical conjugation or genetic fusion. HSA has a plasma half-life of around 21 days owing to its interaction with the neonatal Fc receptor (FcRn) expressed in endothelial cells of blood vessels, which rescues circulating HSA from lysosomal degradation. We have conjugated GLP-1 to C34 of native sequence recombinant HSA (rHSA) and two rHSA variants; one with increased and one with decreased binding affinity to *h*FcRn. We have investigated the impact of conjugation on FcRn binding affinities, GLP-1 potency and pharmacokinetics, combined with the solution structure of the rHSA variants and GLP-1 albumin conjugates. The solution structures, determined by small angle X-ray scattering, show the GLP-1 pointing away from the surface of rHSA. Combining the solution structures with the available structural information on the FcRn and GLP-1 receptor (GLP-1R) obtained from X-ray crystallography, we can explain the observed *in-vitro* and *in-vivo* behaviour. We conclude that the conjugation of GLP-1 to rHSA does not affect the interaction between rHSA and FcRn, while the observed decrease in the potency of GLP-1 can be explained by a steric hindrance of GLP-1 binding to its receptor.

Abbreviations: HSA: *human* serum albumin; rHSA: recombinant *human* serum albumin; GLP-1: glucagon-like peptide 1; WT: wild-type; DPP-VI: dipeptidyl-peptidase-IV; IgG: Immunoglobulin G; NMR: nuclear magnetic resonance; FcRn: neonatal Fc receptor; SAXS: small angle X-ray scattering. GLP-1-PEG-mal: HEGTFTSDVSSYLEGQAAKEFIAWLKGR-K-(8-amino-3,6,dioxaoctanoyl-maleimidopropionyl)); NMRI: naval medical research institute; PK: pharmacokinetics

Keywords: GLP-1, glucagon-like peptide 1, albumin, HSA, SAXS, small angle X-ray scattering, pharmacokinetics, pk, FcRn binding, albumin conjugation, half-life extension

## INTRODUCTION

According to the International Diabetes Federation <sup>1</sup> the number of diabetes patients, which in 2015 was 415 million world wide will have increased to 642 million people in 2040. Since the approval of Byetta<sup>®</sup> by the US Food and Drug administration in 2005 as the first in class glucagon-like peptide 1 (GLP-1) receptor agonist, GLP-1 has been successfully used for the treatment of diabetes providing effective control of blood glucose levels, lowering of systolic blood pressure and reduction of body weight <sup>2</sup>.

GLP-1 is a 30 amino acid (7-36-amide; UniProt: P01275) peptide incretine hormone and its secretion is stimulated by food intake <sup>3</sup>, resulting in an amplification of the insulin response <sup>4,5</sup>. The reported plasma half-life of GLP-1 is, however, less than 3 minutes <sup>6-9</sup> wherefore the native peptide is unsuitable as a drug candidate. There are two main reasons for the short half-life; due to the small size (molar mass of 3.3 kDa) GLP-1 is cleared rapidly by renal filtration <sup>8</sup>. Furthermore, a specific inactivation mechanism exists as GLP-1 is sensitive to dipeptidyl-peptidase-IV (DPP-IV) hydrolysis and is therefore rapidly inactivated in human plasma by truncation of the N-terminal His-Ala forming the inactive 9-36-amide degradation product <sup>10</sup>. Studies using continuous administration by intravenous infusion of GLP-1, indicate a clinical relevance of GLP-1 as drug candidate when the action of the peptide is sufficiently extended <sup>11</sup>, and three different approaches have been pursued to extend the circulatory half-life of GLP-1: Reduction of the sensitivity towards DPP-IV degradation, decrease of the rate of passive renal clearance and third, mobilization of active recycling mediated by the FcRn. In Table S1, we show a selection of GLP-1 variants with their reported half-life. Reduction of sensitivity towards proteolytic inactivation by DPP-IV significantly extends the half-life of GLP-1 from minutes to hours. Examples of this approach are the development of drugs such as exenatide <sup>12</sup> and lixisenatide <sup>13</sup>, where the half-life was successfully increased from a few minutes to 2.4 and 3-4 hours, respectively, allowing for twice and once daily administration. Although a lowering of the DPP-IV induced degradation results in a ~50 fold increase in the half-life, renal filtration is still very efficient in clearing the peptides. Increasing size to diminish renal clearance will additionally increase the half-life of GLP-1, and this approach has been utilized in the development of several drug candidates such as liraglutide, which is a human GLP-1 analogue lipidated at position 16 allowing for complex formation with endogenous HSA. The lipidation additionally induces a concentration independent multimerization of the peptide resulting in a 6-8 fold increased size to approximately 30 kDa <sup>14</sup>. The lipidation results in a plasma half-life of 11-13 hrs <sup>15</sup>. However, it is unclear which of the species, the HSA-liraglutide complex or the liraglutide multimer, that are pharmacologically relevant accounting for observed extension of the half-life. Another approach to increase the size is used in LY2428757. Here, GLP-1 is pegylated resulting in a half-life of 2.5 days in cynomolgus monkey<sup>16</sup>. A similar half-life of 2.5 days in cynomolgus monkey was achieved from XTENylation by fusion of an unstructured recombinant polypeptide of 864 amino acids to exenatide <sup>17</sup>.

Additional prolongation of half-life is achieved by covalent attachment of exenatide to the Fc domain of Immunoglobulin G (IgG) <sup>18</sup> or to rHSA <sup>19</sup>. Both IgG and HSA have an extraordinary long half-life of 21 days. The long half-life is a result of an active rescue mechanism where HSA <sup>20-22</sup> and IgG <sup>23-26</sup> are captured by the FcRn and recycled. FcRn rescues the proteins in the endosomes after

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5 pinocytosis through a strong interaction triggered by the relatively low pH (~pH 6-6.5) in this cellular  
6 compartment. Binding to FcRn prevents HSA and IgG from entering into the lysosomal pathway for  
7 destruction. Instead the proteins are released into the extracellular space triggered by an increase in  
8 pH (~ pH 7.4). An extensive review on albumin's inherent properties making it an efficient drug  
9 delivery platform is given in Sleep (2015)<sup>27</sup>. Mustering of the FcRn recycling mechanism by covalent  
10 attachment to the Fc domain of IgG or to rHSA, further extends the half-life by a factor of ~2.5.  
11 Dulaglutide, an exenatide-Fc fusion protein, has thus been reported to have a circulatory half-life of  
12 4 days. Albiglutide, a (GLP-1 analogue)<sub>2</sub>-albumin fusion and CJC-1134, an exenatide-albumin  
13 conjugation have been reported to have a half-life of 6<sup>28,29</sup> and 8<sup>30</sup> days, respectively. Semaglutide  
14 <sup>31</sup> is a once-weekly GLP-1 analogue with two amino acid substitutions, giving rise to decreased *in-*  
15 *vivo* degradation by DPP-IV, and lipidation at position number 26, allowing for complex formation  
16 between endogenous HSA and semaglutide, resulting in a plasma half-life of approximately 7 days  
17 <sup>32</sup>. This compares to the half-life observed of the GLP-1 analogues that are covalently linked to rHSA  
18 and suggests to us that the complex formed is resilient and enabling FcRn recycling of the complex.  
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24 A potential concern is that conjugation of drugs to albumin can have an adverse effect on the binding  
25 of albumin to FcRn resulting in limited half-life extension, and also resulting in a decreased potency  
26 of the conjugate by affecting the binding of the drug to its target. The latter can be assessed by three-  
27 dimensional (3-D) structures of drug-target complexes providing an atomistic insight. 3-D crystal  
28 structures of GLP-1 variants conjugated to HSA are not available. However, some structural insight  
29 is provided by the solution structures of GLP-1 (pdbid: 1DOR)<sup>33</sup> and exendin-4 (pdbid: 1JRJ) that  
30 both show a helical peptide with flexible N-and C-terminals.  
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35 The 3-D structures of the extracellular part of the GLP-1R in complex with exendin-4 (pdb ids: 3C5T,  
36 3C59)<sup>34</sup>, GLP-1 (pdbid: 3IOL)<sup>35</sup> and semaglutide (pdbid: 4ZGM)<sup>32</sup> show similar binding patterns  
37 with both hydrophobic and hydrophilic interactions being responsible for the binding and that the C-  
38 terminal part of the helix binds to the extracellular part of the receptor. A two-step binding mechanism  
39 of GLP-1 to the receptor has been proposed involving initial binding of the C-terminal of the peptide  
40 to the extracellular part of the GLP-1R. This facilitates the interaction of the N-terminal of GLP-1 to  
41 the core part of the GLP-1R (reviewed by Hoare (2005)<sup>36</sup>). The receptor is a seven-transmembrane  
42 G protein-coupled receptor<sup>37</sup> and the structure of the full-length receptor with a peptide agonist bound  
43 has been solved by X-ray crystallography<sup>38</sup> (pdbid: 5NX2).  
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48 We set out to study the effect of conjugating GLP-1 to C34 of three variants of rHSA. Wild type  
49 rHSA (WT-albumin), a variant known to have high binding affinity to FcRn (HB-albumin; K573P)<sup>39</sup>  
50 and a variant known to have very low binding affinity to FcRn (NB-albumin; K500A)<sup>40</sup>. The FcRn  
51 binding kinetics, the GLP-1R agonist activity in  $\beta$ TC6 pancreatic tumour cells and the  
52 pharmacokinetics in mice were determined. These results were complimented by structural models  
53 of the GLP-1 albumin conjugates derived from small angle X-ray scattering (SAXS) allowing  
54 modelling of the molecular interactions explaining the experimental observations.  
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## 58 METHODS

### 59 *Albumin variants*

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5 WT-, NB-, and HB-albumin were produced by secretion from yeast as described elsewhere <sup>40</sup>,  
6 followed by a 2-step purification using AlbuPure<sup>®</sup> (ProMetic BioSciences Ltd UK) and  
7 diethylaminoethyl weak anion exchange Sepharose Fast Flow (GE Healthcare).  
8

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10 GLP-1 with a C-terminal maleimide group was purchased from PolyPeptide Laboratories France SAS  
11 (Sequence of maleimide coupled GLP-1: HEGTFTSDVSSYLEGQAAKEFIAWLKGR-K-(8-  
12 amino-3,6,dioxaoctanoyl-maleimidopropionyl)) (GLP-1-PEG-mal). The maleimide group reacts  
13 with the free C34 of rHSA hereby conjugating GLP-1 to rHSA. The three GLP-1-PEG-albumin  
14 variants were GLP-1-PEG-WT-albumin, GLP-1-PEG-NB-albumin and GLP-1-PEG-HB-albumin.  
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17 The sequence and identity of all compounds were confirmed by MS (data not shown).  
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20 Buffer components and salts for the purifications were purchased from Sigma Aldrich. All solutions  
21 were prepared using water for injection (WFI) (HyClone WFI, Thermo scientific). The conjugation  
22 reaction was performed in PBS (Medicago, Sweden) at pH 7.1 with 1.5 molar excess of rHSA to  
23 GLP-1-PEG-mal. The reaction was performed over night at room temperature with gentle shaking  
24 and terminated by addition of 0.5 volume WFI followed by pH adjustment to 5.3 with acetic acid.  
25 Unconjugated GLP-1-PEG-mal was removed by AlbuPure<sup>®</sup> matrix (ProMetic BioSciences)  
26 chromatography; unconjugated rHSA and GLP-1 albumin conjugates were eluted with 50 mM  
27 ammonium-acetate, 10 mM octanoate pH 7.0 <sup>41</sup>. To the affinity purified material, ammonium sulphate  
28 was added to a final concentration of 0.5 M for separation of unconjugated and conjugated rHSA on  
29 a HiTrap Butyl sepharose HP column (GE Healthcare) equilibrated in 0.5 M (NH<sub>4</sub>)<sub>2</sub>SO<sub>4</sub>, 20 mM Na-  
30 phosphate, 5 mM Na-octanoate pH 7.0. GLP-1-PEG-albumin was eluted with a linear gradient from  
31 0.5 M (NH<sub>4</sub>)<sub>2</sub>SO<sub>4</sub>, 20 mM Na-phosphate, 5 mM Na-octanoate pH 7.0 to WFI. Mono-conjugates eluted  
32 at approx. 0.25 M (NH<sub>4</sub>)<sub>2</sub>SO<sub>4</sub>. The purified mono-conjugate was added 1/10 volume of 10× PBS to  
33 control pH. The conjugation was stabilized by hydrolysis (ring-opening) of the maleimide ring <sup>42</sup> by  
34 addition of glycine to 25 mM and pH adjustment to 9.0. The hydrolysis was performed for 20 hrs at  
35 room temperature and terminated by neutralizing to pH 7.0. The HiTrap Butyl sepharose HP  
36 purification was repeated to obtain the stabilized mono-conjugate, and the samples were transferred  
37 into PBS pH 7.4 using VivaSpin<sup>®</sup> 20 (Sartorius Stedim) with a 30K membrane for *in-vitro* and *in-*  
38 *vivo* studies.  
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#### 46 *Octet/ FcRn binding kinetics*

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49 Biolayer interferometry on an Octet Red96 system (PALL/ForteBio) was used to characterize the  
50 binding kinetics of the GLP-1-PEG-albumin conjugates. Biotinylated *mouse* and *human* FcRn  
51 (*mFcRn* and *hFcRn*) were purchased from Immunitrack, Denmark, and immobilized on streptavidin  
52 coated biosensors (PALL/ForteBio) in PBS pH 7.4 supplemented with 0.01% Tween-20.  
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55 The sensors were pre-blocked to minimize non-specific binding by 5 min soaking in rHSA diluted to  
56 0.5 mg/mL in 25 mM Na-acetate, 25 mM NaH<sub>2</sub>PO<sub>4</sub>, 150 mM NaCl, 0.01% Tween-20 pH 5.5,  
57 followed by 5 min. rinse in the same buffer without rHSA, and subsequently in milliQ water. The  
58 sensors were prepared for storage by soaking in 15% sucrose and air drying.  
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5 For kinetic characterization, a 7-step two fold dilution series was prepared in 25 mM Na-acetate, 25  
6 mM NaH<sub>2</sub>PO<sub>4</sub>, 150 mM NaCl, 0.01% Tween-20 at pH 5.5 starting at 100 µg/mL for pH 5.5 except  
7 for NB-albumin and GLP-1-PEG-NB-albumin starting at 400 µg/mL. The binding kinetics were  
8 performed at 30°C with a 120 sec. association phase and 300 sec. dissociation phase. The sensors  
9 were regenerated with PBS pH 7.4 and equilibrated in 25 mM Na-acetate, 25 mM NaH<sub>2</sub>PO<sub>4</sub>, 150 mM  
10 NaCl, 0.01% Tween-20 at the specified pH between the different samples. All data were referenced  
11 with FcRn-streptavidin sensors in buffer without rHSA or GLP-1 albumin conjugates. Data analysis  
12 was performed using the Octet data analysis software ver. 8.0 (PALL/ForteBio) using curve fitting to  
13 a 1-1 model for estimation of kinetic parameters. For the variants with a fast off-rate only the first 30  
14 sec of the dissociation phase were included for curve fitting to minimize the contribution of un-  
15 specific binding to the sensors.  
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### 20 21 *SAXS solution structure determination*

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23 SAXS measurements were performed at the MAX IV laboratories at beamline I911-SAXS, Lund,  
24 Sweden <sup>43</sup>. The sample detector distance and the direct beam position were calibrated using silver  
25 behenate. Parameters are listed in Table S2a. Measurements on pure water were used to get the data  
26 on an absolute scale. Buffers were measured before and after each sample and averaged before  
27 subtraction. The sample size was approximately 50 µL using an automated flow cell. Measurements  
28 were performed on a series of samples as outlined in Table S2b.  
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32 All calibrations and corrections of the SAXS data were done using the in-house software Bli911-4 <sup>43</sup>.  
33 Buffer averaging and subsequent subtraction prior to data analysis were done in Primus <sup>44</sup>.  
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35 The difference between the scattering curves of GLP-1 albumin conjugates and rHSA variants was  
36 qualitatively compared by comparing the curves individually by  $\chi^2$  using the online similarity tool  
37 created by the Sibyls group <sup>45</sup>.  
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40 The ATSAS program package version 2.4 <sup>46</sup> was used for further data treatment and analysis.  
41 Evaluation of the Guinier region was performed within Primus. The pair distribution function,  $p(r)$ ,  
42 was evaluated using the interactive program GNOM <sup>47</sup>. The flexibility was analysed using the  
43 dimensionless Kratky plot <sup>48</sup> where  $(qR_g)2I(q)/I(0)$  is displayed as a function of  $qR_g$ , making the  
44 plot independent of protein size and intensity scale.  
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48 3D crystal structures of HSA exist with and without fatty acids bound. We compared the SAXS  
49 measurements of the rHSA variants to the defatted structure (pdbid: 1AO6 <sup>49</sup>) and a fatty acid bound  
50 structure (pdbid: 1BJ5 <sup>50</sup>) using Crysol <sup>51</sup>. The best match was found with pdbid 1AO6, which was  
51 used for further modelling. The linker between rHSA and GLP-1 was modelled by 7 glycine residues,  
52 approximating the chemical nature of the PEG linker.  
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56 Rigid body modelling of the GLP-1-PEG-albumin conjugates with the linker between rHSA (pdbid:  
57 1AO6 <sup>49</sup>) and GLP-1 (pdbid: 1D0R <sup>52</sup>) was done in BUNCH <sup>53</sup>. Due to variations in the models  
58 produced by BUNCH, the flexibility of the conjugates was evaluated using the ensemble optimization  
59 method (EOM) <sup>54,55</sup>.  
60

### GLP-1 activity assay

*In vitro* biological activities of GLP-1, GLP-1-PEG-mal and GLP-1-PEG-WT-albumin conjugates were determined by an agonist-binding assay using  $\beta$ TC6 pancreatic tumour cells. Cells were incubated with titrations of test compounds or 10 nM control GLP-1 (7-37) for 10 minutes at room temperature, and cAMP was measured by homogeneous time resolved fluorescence (HTRF) as described in <sup>11</sup>. Results were normalized to control GLP-1 and EC<sub>50</sub> values were calculated from fits of dose-response curves (four parameters variable slope).

### Pharmacokinetics in NMRI WT mice

The pharmacokinetic study was approved by the ethical committees at both BioAdvice (Ølstykke, Denmark) and Novozymes A/S. The study was performed at BioAdvice. 5 mg/kg of GLP-1-PEG-WT-albumin, GLP-1-PEG-HB-albumin or WT-albumin were administered intravenously to NMRI mice (female, aged 8-10 weeks, weight between 20 and 22 g, 10 mice/compound, 5 mice/time point). Blood samples were collected from the tail vessel in time intervals of predose 0.5, 1, 2, 4, 8, 12, 24, 48, 72, 96, 120, 144, 168 and 192 hours. Upon collection, the blood samples were kept at 4°C for a maximal duration of 3 hours followed by centrifugation at 14,000G for 15 min at 20°C and stored at -80°C prior to bioanalysis. Serum concentrations were determined using an AlphaLISA method employing a commercial HSA kit (AL296C, Perkin Elmer, MA, USA) combined with a monoclonal anti-GLP-1 biotinylated monoclonal antibody (Ab121072, Abcam) to detect both albumin and GLP-1 moieties simultaneously; for albumin alone, the albumin kit was used. The standard curve on each plate was fitted to a four-parameter nonlinear regression model, and the serum concentrations were calculated at each time point using the dilutions that fell within the linear range of the standard curve. Mean serum concentration profiles were subjected to non-compartmental pharmacokinetic analysis using WinNonLin 6.3. Nominal time points and doses were used, and all data points were equally weighted in the analysis.

## RESULTS

### Pharmacology

The kinetic parameters as determined by Biolayer interferometry are summarized in Table 1 and the sensorgrams are shown in Figure S1. Several things may be noticed. First, an increased binding to FcRn is seen by HB-albumin compared to WT-albumin by a factor of 20 due to an ~10-fold decrease in  $k_{off}$ . Second, the data show that conjugation of GLP-1 to C34 in any of the variants result in similar  $K_D$ ,  $k_{off}$  and  $k_{on}$ . This indicates that neither *hFcRn* nor *mFcRn* binding is hampered by conjugation. Third, if we compare the *human* WT-albumin and the *mouse* albumin, it is clear that the mouse protein binds better to both *hFcRn* and *mFcRn*, similar to what has been observed by others<sup>56</sup>. We found a factor of 10 in difference for *mFcRn* and a factor of 3 for *hFcRn*. In addition, it is clear that human WT-albumin binds much better to *hFcRn* than to *mFcRn* (548.7 nM vs. 4702.0 nM). The  $K_D$  values summarized in Table 1 are in the same range as earlier reported when measured using the Biolayer interferometry method (in nM): WT-albumin (*hFcRn*: 797.9±155.0, *mFcRn*: 5391.0±367.7), HB-



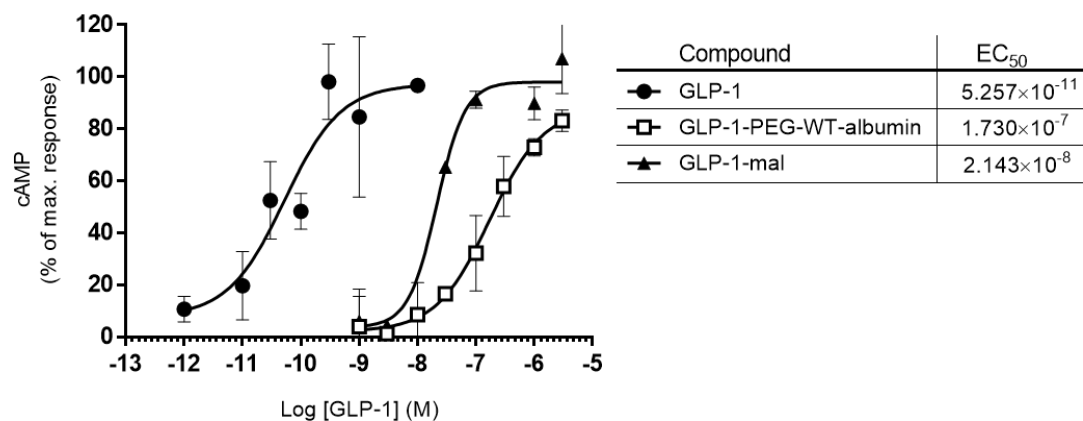
albumin (*hFcRn*:  $31.5 \pm 9.8$ , *mFcRn*:  $764.3 \pm 17.5$ ) and mouse albumin (*hFcRn*:  $74.6 \pm 13.4$ , *mFcRn*:  $314.9 \pm 12.1$ )<sup>57</sup>.

**Table 1 Octet Binding kinetics – affinity towards the *human* and *mFcRn* receptor**

	<i>hFcRn</i>			<i>mFcRn</i>		
	$K_D \pm SD$ (nM)	$k_{on} \pm SD$ ( $10^3/Ms$ )	$k_{off} \pm SD$ ( $10^3/s$ )	$K_D \pm SD$ (nM)	$k_{on} \pm SD$ ( $10^3/Ms$ )	$k_{off} \pm SD$ ( $10^3/s$ )
WT-albumin	$548.7 \pm 90.2$	$31.5 \pm 2.8$	$17.1 \pm 1.4$	$4702.0 \pm 1096.5$	$11.7 \pm 3.9$	$52.0 \pm 9.5$
GLP-1-PEG-WT-albumin	$856.5 \pm 94.9$	$25.5 \pm 2.8$	$21.7 \pm 1.4$	$3506.7 \pm 910.2$	$11.7 \pm 2.6$	$39.6 \pm 5.5$
NB-albumin	Low binding			Very low binding		
GLP-1-PEG-NB-albumin	Low binding			Very low binding		
HB-albumin	$25.2 \pm 4.3$	$35.4 \pm 3.9$	$0.9 \pm 0.1$	$1774.0 \pm 299.7$	$20.1 \pm 3.0$	$34.9 \pm 1.0$
GLP-1-PEG-HB-albumin	$26.1 \pm 2.7$	$40.3 \pm 2.1$	$1.0 \pm 0.1$	$1324.7 \pm 418.7$	$21.5 \pm 4.9$	$27.1 \pm 1.5$
Mouse albumin	$191.6 \pm 31.4$	$22.6 \pm 1.6$	$4.3 \pm 0.4$	$486.2 \pm 125.2$	$21.3 \pm 4.0$	$10.1 \pm 0.7$

### GLP-1-PEG-albumin conjugates potency and pharmacokinetics

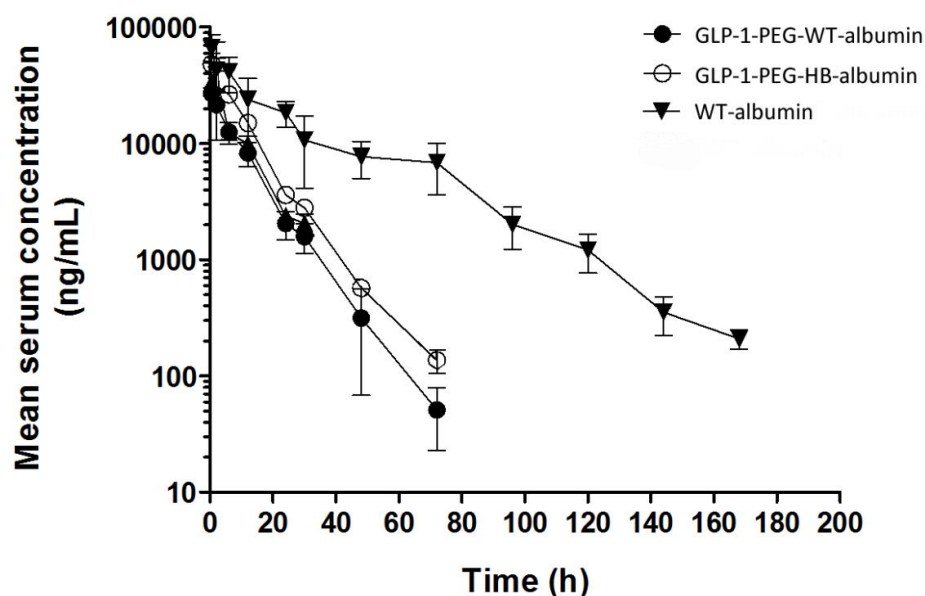
GLP-1-PEG-WT-albumin potency was investigated and compared to that of unconjugated GLP-1 and of GLP-1-PEG-mal (Figure 1). The *in vitro* activity of GLP-1 and its conjugated counterparts was measured by generation of cAMP after stimulation of  $\beta$ TC6 pancreatic tumour cells. When conjugated to PEG-albumin, the potency of GLP-1 was reduced by 3-4 orders of magnitude, seen by a shift in  $EC_{50}$  from  $5.257 \times 10^{-11}$  to  $1.730 \times 10^{-7}$  (See table insertion in Figure 1). A smaller decrease in potency was found when GLP-1 was conjugated to PEG-mal alone.



**Figure 1 In vitro biological activity of GLP-1, GLP-1-PEG-mal and GLP-1-PEG-WT-albumin in  $\beta$ TC6 cells. cAMP response is shown and data represent the means  $\pm$ SD of replicates.**

Mouse pharmacokinetics of rHSA alone and GLP-1 linked albumins are shown in Table 2. Reported GLP-1 half-life in mice is approx. 2 min<sup>58</sup>, while the half-life of rHSA is approx. 22 hours<sup>39</sup>. The latter compares well to the half-life found in this study (Table 2). Linking GLP-1 to WT-albumin is shown to extend the half-life of GLP-1 significantly (Figure 2), and the half-life increases from 0.03 hours to 8.5 hours corresponding to a 280 fold increase. Replacing WT-albumin with the high FcRn

binding affinity variant HB-albumin extends the half-life of GLP-1 330-fold (to 9.9 hours; Table 2). The HB-albumin variant also increases the systemic exposure of the drug (note the increase in AUC for GLP-1-PEG-HB-albumin). These results emphasize the benefits of using rHSA and rHSA variants to improve the pharmacokinetics of receptor agonists such as GLP1.



**Figure 2** Pharmacokinetic profiles of WT-albumin, GLP-1-PEG-WT-albumin and GLP-1-PEG-HB-albumin in NMRI mice administered 5mg/kg, i.v. Data are based on ten mice.

**Table 2** Pharmacokinetics in Mice after Single IV Administration of 5 mg rHSA variant/kg.  $T_{max}$ : time to reach maximum serum concentration,  $C_{max}$ : maximum concentration after administration,  $AUC_{0-\infty}$ : area under the curve,  $t_{1/2}$ : elimination half-life,  $V_z$ : volume of distribution,  $Cl$ : clearance; volume of plasma from which a drug is eliminated per unit time.

Compound	$T_{max}$ (h)	$C_{max}$ ( $\mu\text{g/mL}$ )	$AUC_{0-\infty}$ ( $\text{h}\cdot\mu\text{g/mL}$ )	$t_{1/2}$ (h)	$V_z$ ( $\text{mL/kg}$ )	$Cl$ ( $\text{mL}\cdot\text{kg}^{-1}\cdot\text{h}^{-1}$ )
GLP-1	-	-	-	0.03 <sup>58</sup>	-	-
WT-albumin	0.5	66	1481	21.5	104	3.4
GLP-1-PEG-WT-albumin	0.5	27	276	8.5	223	18.1
GLP-1-PEG-HB-albumin	0.5	48	494	9.9	143	10.1

## SAXS

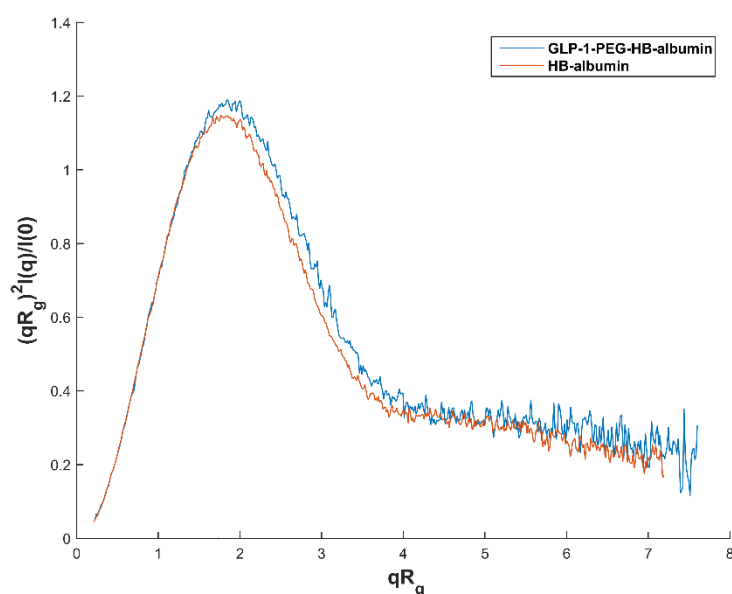
All scattering profiles are shown in Figure S2 and the data analysis parameters are listed in Table S3. The three rHSA variants have similar scattering curves and the three GLP-1 albumin conjugates have similar scattering curves. This is further verified by the similarity test shown in Figure S3, which also establishes that the GLP-1 albumin conjugates are structurally different from the unconjugated albumins.

All GLP-1-PEG-albumin conjugates have larger radius of gyration ( $R_g$ ) than the rHSA variants as shown in Table 3. This indicates that the conjugated GLP-1 somewhat protrudes away from the rHSA instead of interacting with the protein surface. This is further verified by the results from the

dimensionless Kratky plots shown in Figure 3, where GLP-1-PEG-HB-albumin is compared to the HB-albumin variant. The plots show how the conjugate is larger as the maximum of the curve is shifted to higher  $qR_g$  values.

**Table 3**  $R_g$  determined from Guinier analysis using Primus [51].

Compound (1 mg/ml)	$R_g$ (nm)	Standard deviation	Compound (1 mg/ml)	$R_g$ (nm)	Standard deviation
WT-albumin	2.96	0.19	GLP-1-PEG-WT-albumin	3.16	0.18
NB-albumin	3.00	0.29	GLP-1-PEG-NB-albumin	3.19	0.18
HB-albumin	2.98	0.18	GLP-1-PEG-HB-albumin	3.18	0.26



**Figure 3** Dimensionless Kratky plot of GLP-1-PEG-HB-albumin compared to HB-albumin

The structure of GLP-1 was taken as an ensemble representative from the pdb entry 1D0R. This structure of *human* GLP-1 is an NMR structure determined at pH 2.5, while a crystal structure in complex with the extracellular part of the GLP-1R (pdbid: 3IOL) is at pH 6.9. These two structures show very similar secondary structure of GLP-1. Based on this there is no reason to believe that GLP-1 should change structure at pH 7.4. BUNCH<sup>53</sup> gave models with  $\chi^2$  values in the range from 3.48 - 3.88 for the GLP-1-PEG-HB-albumin models. Results from the 10 independent BUNCH simulations from the GLP-1-PEG-HB-albumin are shown in Figure 4. The NB and the WT variants gave similar results.



**Figure 4** GLP-1-PEG-HB-albumin shown in gray (domain I: medium gray, domain II: dark gray, domain III: light gray) and the conjugated GLP-1s are shown in pink as 10 representative structures.

Due to the semi-flexible nature of the GLP-1 albumin conjugates observed from BUNCH and the dimensionless Kratky plot, modelling was performed again but this time with the Ensemble Optimization Method (EOM)<sup>54,55</sup>. EOM was run in two different ways: One with the structure of GLP-1 set as a helix, i.e. the same PDB structure as above, and a flexible linker and one where the entire GLP-1 and the linker are flexible, though with geometry optimized backbone angles. The results are shown in Figure S4, which show that the helical structure of GLP-1 is a good approximation, as the  $R_g$  and  $D_{max}$  distributions are very similar between the two methods, and the  $\chi^2$  values were 1.150 and 1.145 respectively for the GLP-1-PEG-albumin conjugates, confirming the flexibility of the GLP-1 position.

## DISCUSSION

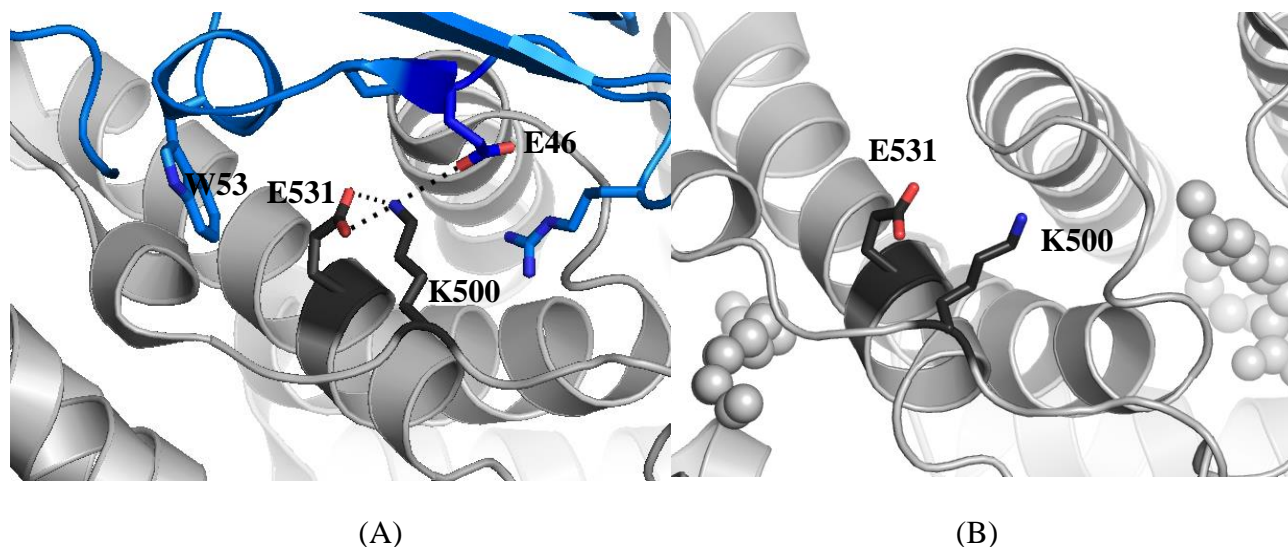
The rHSA variants were previously shown to have different affinities for the FcRn<sup>39,40</sup>, which was confirmed by the  $K_D$  data in Table 1 showing increased binding for HB-albumin and reduced binding for NB-albumin compared to WT-albumin. Two crystal structures exist of the FcRn:rHSA complex. A complex of a quadruple rHSA variant V418M/T420A/E505G/V547A in complex with *h*FcRn (pdbid: 4K71<sup>59</sup>) and a complex between WT-rHSA and *h*FcRn (pdbid: 4N0F<sup>60</sup>). The pH dependent binding of HSA to the FcRn facilitates the recycling of HSA. HSA undergoes conformational changes upon binding, which is a major movement of domain III and a smaller movement of domain I with respect to domain II. The domain positions of HSA are indicated in Figure 7. It is discussed if the pH dependent binding is governed primarily by FcRn H161, which is the only histidine residue observed in the interface between HSA and *h*FcRn<sup>60</sup> or if it is governed by a number of conserved histidine

residues in FcRn and HSA.<sup>40</sup> Furthermore, it is observed that two conserved tryptophan residues, W53 and W59 in the *h*FcRn  $\alpha$ -chain, are deeply docked into the fatty acid binding sites in HSA suggesting that binding of fatty acids to HSA hampers recycling<sup>59</sup> and that the interface between HSA and *h*FcRn mainly is governed by hydrophobic interactions.

The SAXS experiments performed at pH 7.4 confirm that the solution structure of the two variants (NB-albumin and HB-albumin) and the WT-albumin are indistinguishable from each other as the scattering curves are identical (as shown in Figures S2 and S3).

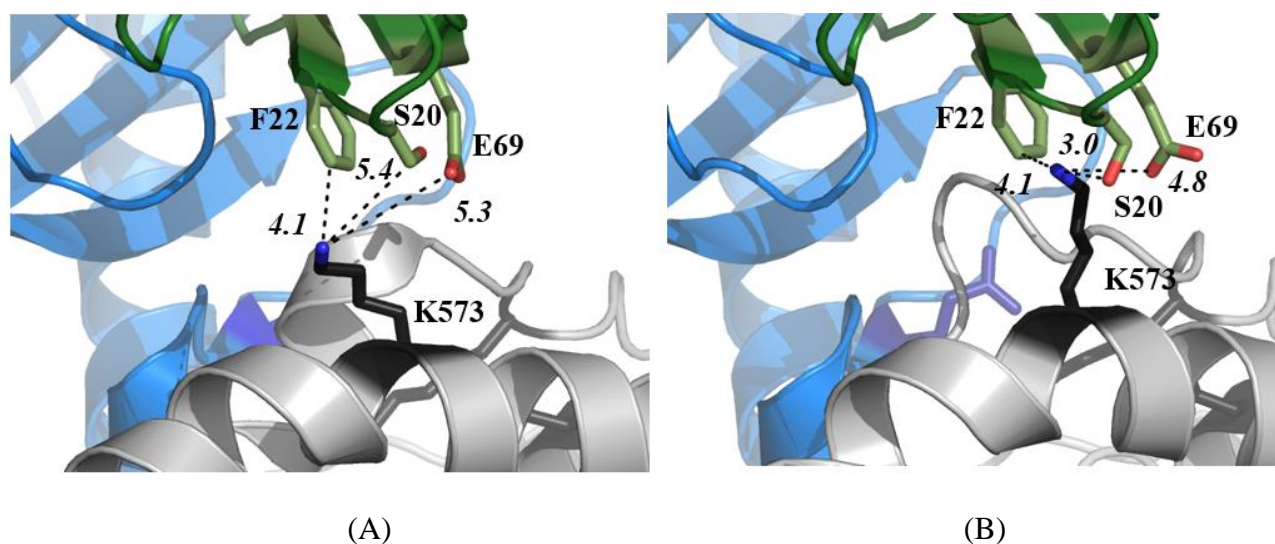
The GLP-1-PEG-albumin conjugates also had similar scattering curves and could all be modelled using GLP-1 protruding from the surface of rHSA with the rHSA conformation found in the defatted structure. Flexibility of the linker was confirmed by comparing BUNCH and EOM results, though limited to a cone area of an approximate diameter of 40 Å, as may be deduced from Figure 4.

Both the NB-albumin and the HB-albumin have amino acids changed on the surface of domain III in rHSA. The analysis of the structural impact of the variants is hampered by the fact that differences are observed in the two complex structures (pdbids: 4N0F or 4K71) in exactly this area of the structure: The NB-albumin K500A has a lysine changed to an alanine on the surface of domain III, involved in the FcRn binding. The K500 in the native structure of the rHSA-FcRn complex (pdbid: 4N0F; Figure 5, (A)), is making an intramolecular salt bridge to rHSA E531. This salt bridge is not present in the fatty acid bound HSA structure (pdbid: 1BJ5; Figure 5 (B)) and could therefore be important for the domain movement, facilitating FcRn binding. Furthermore, rHSA K500 also forms a salt bridge with FcRn  $\alpha$  E46. These salt bridges are in the proximity of the pocket where the FcRn W53 is binding. It is plausible that breaking these salt bridges will make it less favourable for W53 to bind, affecting complex formation (see Figure 5).



**Figure 5** rHSA K500, rHSA E531 (black) and FcRn  $\alpha$  E46 (dark blue) showing electrostatic interaction in the rHSA-FcRn structure (A): pdbid: 4N0F . rHSA E531 and rHSA K500 do not interact in fatty acid bound rHSA (B): (pdbid: 1BJ5) The gray spheres are myristic acids bound to rHSA. Color code: Gray: rHSA, Blue: FcRn  $\alpha$  chain.

When speculating about binding to FcRn there is no reason to believe that the mechanism for the HB-albumin differs from that found for HSA. The pH dependent binding is believed to be triggered by protonation of one or more histidine residues. This should still be possible in the investigated K573P HB variant. The observed difference in binding is a slightly improved association rate and a slower dissociation rate as indicated by  $k_{on}$  and  $k_{off}$  in Table 1, with retained pH dependent binding as observed by Petersen *et al.*<sup>61</sup>. The HB variant has been changed on the surface of domain III where it interacts with the FcRn  $\beta 2m$  chain. The primates are unique in having a lysine at position 573 – the most common amino acid at this position (and also in mouse) is a proline<sup>59</sup>. Consulting the two available crystal structures of rHSA complexed with FcRn (pdbid:4K71 and pdbid:4N0F) shows that K573 is interacting with S20 and E69 in pdb structure 4K71 (Figure 6 (B)) but not in 4N0F (Figure 6 (A)) where it is bent away from FcRn F22 in the  $\beta 2m$  chain. The global binding mechanism behind the effect of changing K573 is therefore less clear. If steric hindrance with F22 is minimized, it may be rationalized that by changing it to a smaller side chain, binding would be improved. It is also plausible that the proline substitution promotes formation of the hydrophobic interface between HSA and FcRn and maintains the small kink in the HSA helix present at this position.



**Figure 6** Interaction of K573 (black) with S20, F22 and E69 from the  $\beta 2m$  chain of FcRn. (A): pdbid: 4N0F , (B): pdbid: 4K71 . Color code: Gray: rHSA, Green: FcRn  $\beta 2m$  chain and Blue: FcRn  $\alpha$  chain. Distances (Å) are shown in italic and measured in Pymol.

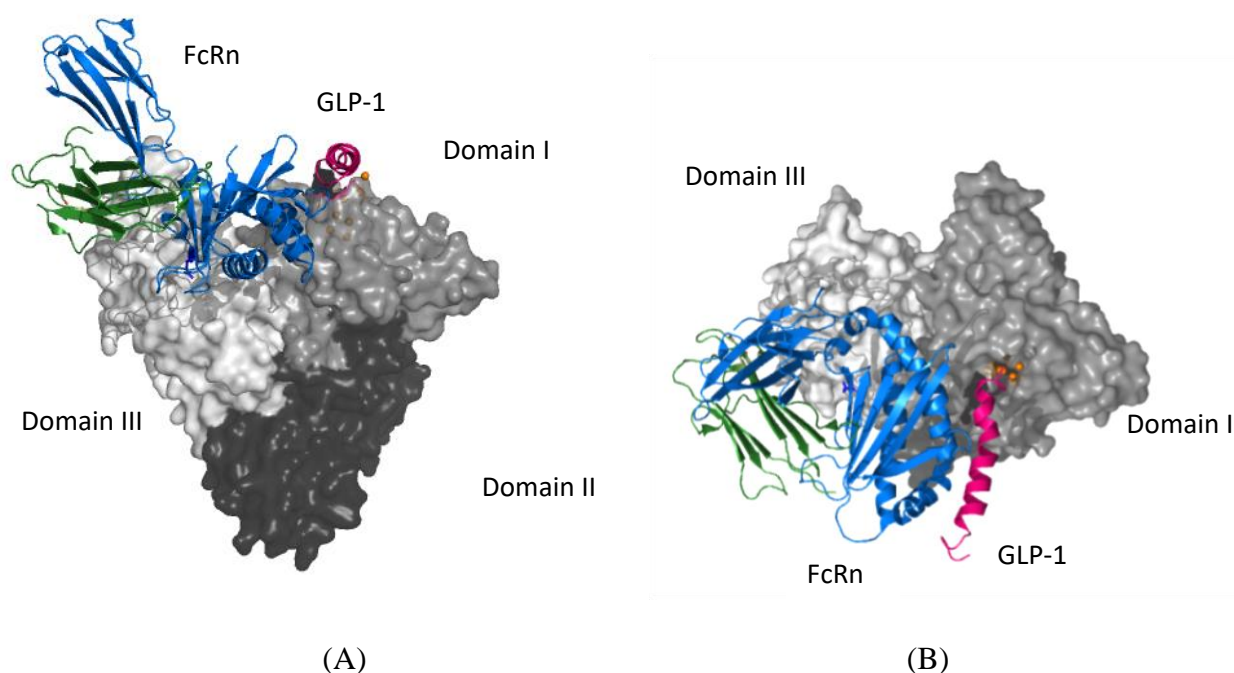
Conjugation of GLP-1 to rHSA had no effect on the FcRn interaction *per se*. FcRn interactions were shown to be unchanged *in-vitro* and this finding was further confirmed *in-vivo*. GLP-1-PEG-HB-albumin showed improved PK compared to GLP-1-PEG-WT-albumin indicating that FcRn-HSA interactions are preserved and can be modulated despite the payload. The overall decrease in half-life (and in this respect the increase in clearance) seen for the GLP-1 albumin conjugates compared to WT-albumin is therefore not caused by FcRn binding impairment. Disposition of GLP-1 and its functional interaction with its receptor, GLP-1R, alter the pharmacokinetics of the conjugates. The bioanalysis of the GLP-1 albumin conjugates was initially performed by employing antibodies against HSA and GLP-1 simultaneously. To confirm that the conjugates are cleared as one molecule, hence GLP-1 does not come off the rHSA while in circulation, we performed bioanalysis of total HSA

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5 content using only HSA antibodies. Both GLP-1 albumin conjugates as well as HSA plasma curves  
6 overlaid (data not shown). These results confirmed the conjugates remain intact and the clearance  
7 mechanisms metabolise the whole molecule simultaneously. As reported for GLP1 and GLP1  
8 agonists, the results suggest the conjugates are cleared via receptor-mediated endocytosis by GLP-  
9 1R<sup>62</sup>. *In-vivo* studies will be relevant to confirm the efficacy of GLP-1 while conjugated to rHSA  
10 and evaluate the full effect on half-life extension.  
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13  
14 It is worth highlighting that these PK studies were performed in mice and therefore limited by cross-  
15 species differences. Cross-species differences constitute a major limitation in pre-clinical  
16 development particularly upon distinct receptor binding kinetics. It has been recognized that caution  
17 should be taken when using rodent models to study the pharmacokinetics of albumin conjugated drugs  
18 <sup>56</sup>. This is also seen in the present results, where the affinity of the *mouse* albumin against the *mFcRn*  
19 is significantly higher than any of the rHSA variants tested (Table 1).  $K_D$  for *mouse* albumin is 2-10  
20 times lower than those determined for the rHSA variants. and the concentration of the tested  
21 compounds is approximately 200-fold lower than the endogenous concentration at the time of the  
22 onset <sup>63</sup>. For this reason significant competition between endogenous *mouse* albumin and rHSA  
23 variants is expected. This translates to the minor improvement achieved for the engineered HB-  
24 albumin against the mouse receptor, i.e. 2-3 fold when compared to the 25-fold improvement against  
25 the human receptor ( $K_D$ , Table 1). Despite the marginal improvements in FcRn binding affinity seen  
26 for the GLP-1-PEG-HB-albumin variant, this variant still outperformed its WT counterpart *in-vivo*  
27 (Table 2). The GLP-1-PEG-HB-albumin showed a slower clearance from plasma leading to 80%  
28 larger exposure and approximately 1.2-fold longer half-life. Based on *in-vitro* binding kinetics and  
29 non-human primate studies evaluating the pharmacokinetics of engineered rHSA variants <sup>39</sup>, we  
30 expect the improvement seen here for the GLP-1-PEG-HB-albumin to render a much more significant  
31 pharmacokinetic improvement in primates.  
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39 In Figure 7, the structure of rHSA in complex with the extracellular domain of the FcRn (pdbid:  
40 4N0F), has been superimposed with a representative model of the GLP-1-PEG-HB-albumin derived  
41 from SAXS data using BUNCH (seen in Figure 4). The conjugation of GLP-1 to C34 is seen to be in  
42 close proximity to the interface area between HSA and FcRn. Apparently, it – even if it is close to  
43 the FcRn – does not sterically hinder the binding of rHSA to the FcRn consistent with the data in  
44 Table 1. Here, it is observed that the affinity and thus the ability to bind to the FcRn seems unchanged  
45 upon conjugation, indicating that the ability to recycle is retained.  
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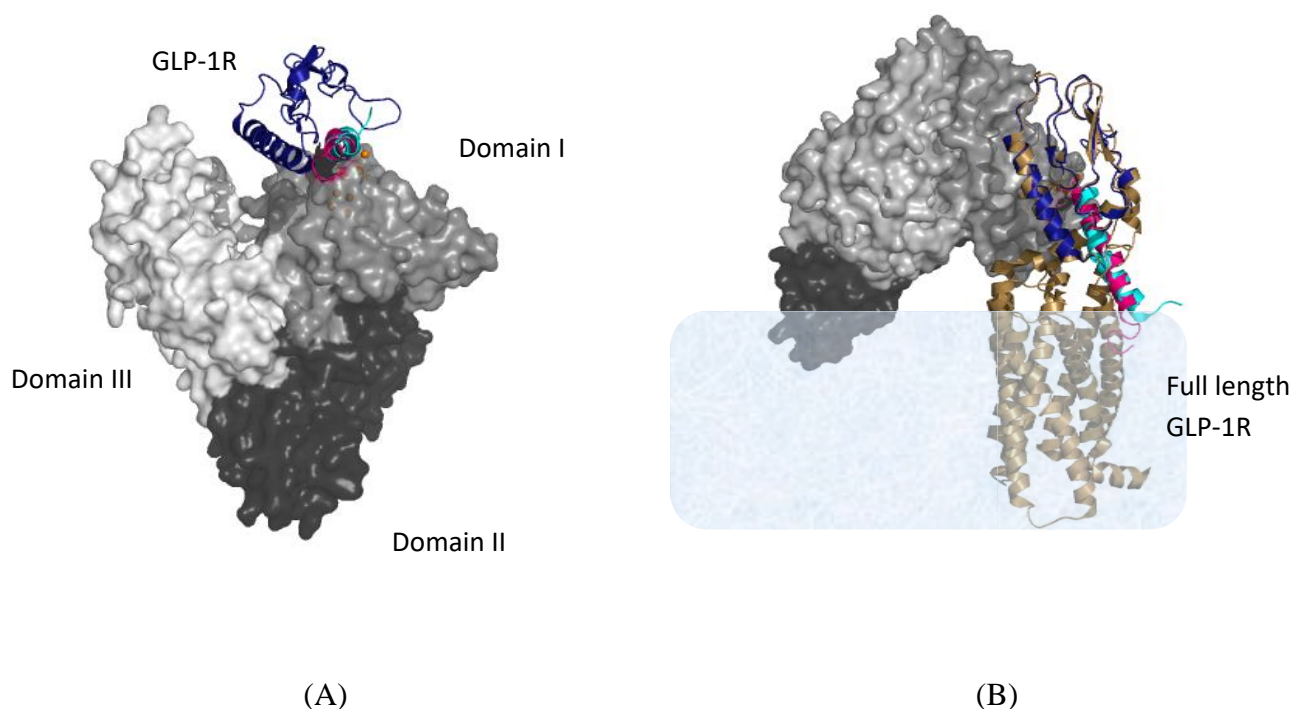
**Figure 7 (A):** The structure of rHSA in complex with the extracellular part of FcRn (pdbid: 4N0F) superimposed on a SAXS-based BUNCH model of GLP-1-PEG-HB-albumin. HSA is displayed in gray (domain I: medium gray, domain II: dark gray, domain III: light gray), FcRn  $\alpha$  in blue and  $\beta$ -2m in green and the conjugated GLP-1 in pink. **(B):** Turned and seen from the top.

In contrast to this, Petersen *et al.*<sup>61</sup> examined the effect on the binding affinity of PEGylated rHSA to FcRn. PEG of sizes 5, 10 and 30 kDa were conjugated to C34 of rHSA. The authors proposed that steric hindrance could be the reason for the observed decreased affinity of the GLP-1 albumin conjugates compared to rHSA.

While the interaction of FcRn with HSA is important for half-life extension of GLP-1, the efficacy is highly dependent on GLP-1 interactions with GLP-1R. From the biological activity assay it was observed that PEG-mal-conjugation to GLP-1 alone lowered the potency by three orders of magnitude for the GLP-1R (Figure 1), and that additionally conjugating rHSA decreased the potency by four orders of magnitude in total. In Figure 8 (A), the structure of GLP-1 in complex with the extracellular part of the GLP-1R (pdbid: 3IOL) has been superimposed with a model of the GLP-1-PEG-HB-albumin. Here, it is seen that the GLP-1 albumin conjugate may bind to the extracellular part of GLP-1R. The full length crystal structure of GLP-1R in complex with a peptide agonist<sup>38</sup> was used to visualize the binding between GLP-1-PEG-albumin and full-length GLP-1R (Figure 8 (B)). Realizing the limitations of this model, it is apparent that albumin within the GLP-1-PEG-albumin conjugate may impact the activity of the GLP-1 moiety, possibly by colliding with the cell membrane, resulting in the lower potency observed for conjugated GLP-1 compared to WT GLP-1. Selis *et al.*<sup>64</sup> observed a decrease in potency of 2-3 orders of magnitude for a number of PEGylated GLP-1 variants. These variants have been PEGylated at GLP-1 positions 11, 23 or 30, which may explain the somewhat smaller decrease in potency compared to our GLP-1-PEG-albumins, which are modified in the C-terminal position 36. This highlights that optimizing the conjugation position is required.



Furthermore, the GLP-1 potency may be regained by changing the conjugation site on rHSA. Our SAXS based models may in this way serve as a valuable source of inspiration for such a design.



**Figure 8 (A):** The structure of GLP-1 (turquoise) in complex with the extracellular part of the GLP-1 receptor (blue), (pdbid: 3IOL) superimposed on a SAXS-based BUNCH model of GLP-1-PEG-HB-albumin. The conjugated GLP-1 is shown in pink, and HSA is displayed in gray (domain I: medium gray, domain II: dark gray, domain III: light gray). **(B):** A rotated version of (A), but with the full-length GLP-1R crystal structure<sup>38</sup> (in bronze) (pdbid: 5NX2) superimposed, and a membrane is indicated as a light blue shadow.

## CONCLUSION

We have studied the effect of conjugating GLP-1 to C34 of WT-, NB- and HB-albumin. The solution structures were determined using SAXS and the results were compared with FcRn binding kinetics, the GLP-1R agonist activity in  $\beta$ TC6 pancreatic tumour cells and the pharmacokinetics in mice. Based on the structure of the GLP-1 albumin conjugates we could model the molecular interactions and explain the experimental observations.

FcRn binding kinetics showed that conjugation of GLP-1 to C34 has limited effect on the *in-vitro* binding to FcRn. In contrast to this the GLP-1R agonist activity in  $\beta$ TC6 cells was decreased by 3-4 orders of magnitude. Similarly, from our studies of PK in NMRI mice we find an increase in half-life of the GLP-1-PEG-albumins compared to GLP-1. Both the unaltered binding to FcRn and the decrease in potency are confirmed by the molecular models derived from the SAXS data, which show that the GLP-1 protrudes out from the rHSA surface with some degree of flexibility. These results show that studying the solution structure using SAXS can be valuable in guiding us to engineer drug conjugation, while in the same time maintaining the integrity of the HSA and its interaction with FcRn.

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