

1 **CONSISTENCY OF FIELD-BASED MEASURES OF NEUROMUSCULAR CONTROL**  
2 **USING FORCE PLATE DIAGNOSTICS IN ELITE MALE YOUTH SOCCER PLAYERS**

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4 **AUTHORS:**

5 **PAUL READ, MSC, ASCC, CSCS\*D**<sup>1</sup>

6 **JON L. OLIVER, PhD**<sup>2,7</sup>

7 **MARK B.A. DE STE CROIX, PhD**<sup>3</sup>

8 **GREGORY D. MYER, PhD, CSCS\*D**<sup>4,5,6,8</sup>

9 **RHODRI S. LLOYD, PhD, ASCC, CSCS\*D**<sup>2,7</sup>

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11 **AFFILIATIONS:**

12 1. School of Sport, Health and Applied Science, St Mary's University, London, UK

13 2. Youth Physical Development Unit, School of Sport, Cardiff Metropolitan University, UK

14 3. School of Sport and Exercise, University of Gloucestershire, UK

15 4. Division of Sports Medicine, Cincinnati Children's Hospital, Cincinnati, Ohio, USA

16 5. Department of Pediatrics and Orthopaedic Surgery, College of Medicine, University of Cincinnati,  
17 Cincinnati, Ohio, USA

18 6. The Micheli Center for Sports Injury Prevention, Boston, MA, USA

19 7. Sport Performance Research Institute, New Zealand (SPRINZ), AUT University, Auckland, New  
20 Zealand

21 8. Department of Orthopaedics, University of Pennsylvania, Philadelphia, Pennsylvania, USA.

22  
23 **CORRESPONDENCE**

24  
25 Name: Paul Read  
26 Address: St Mary's University, Waldegrave Road, Twickenham, London, TW1 4SX  
27 Email: paul.read@stmarys.ac.uk  
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30 **ABSTRACT**

31 Deficits in neuromuscular control during movement patterns such as landing are suggested  
32 pathomechanics that underlie sport-related injury. A common mode of assessment is measurement of  
33 landing forces during jumping tasks; however, these measures have been used less frequently in male  
34 youth soccer players and reliability data is sparse. The aim of this study was to examine the reliability  
35 of a field-based neuromuscular control screening battery using force plate diagnostics in this cohort.  
36 Twenty six pre-peak height velocity (PHV) and twenty five post-PHV elite male youth soccer players  
37 completed a drop vertical jump (DVJ), single leg 75% horizontal hop and stick (75%HOP) and single  
38 leg countermovement jump (SLCMJ). Measures of peak landing vertical ground reaction force  
39 (pVGRF), time to stabilisation (TTS), time to pVGRF, and pVGRF asymmetry were recorded. A test,  
40 re-test design was used and reliability statistics included: change in mean, intraclass correlation  
41 coefficient (ICC) and coefficient of variation (CV). No significant differences in mean score were  
42 reported for any of the assessed variables between test sessions. In both groups, pVGRF and asymmetry  
43 during the 75%HOP and SLCMJ demonstrated largely acceptable reliability ( $CV \leq 10\%$ ). Greater  
44 variability was evident in DVJ pVGRF and all other assessed variables, across the three protocols (CV  
45 range = 13.8 – 49.7%). ICC values ranged from small to large and were generally higher in the post-  
46 PHV players. The results of this study suggest that pVGRF and asymmetry can be reliably assessed  
47 using a 75%HOP and SLCMJ in this cohort. These measures could be utilized to support a screening  
48 battery for elite male youth soccer players and for test re-test comparison.

49

50 **Key Words**

51 Landing force, Injury, Screening

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55 **INTRODUCTION**

56 The demands of soccer impose high physiological demand and an inherent risk of injury due to frequent  
57 repetitions of movements that involve significant musculoskeletal forces and joint loads (10). Existing  
58 injury incidence data in elite male youth soccer indicates that injuries occur mainly in the lower  
59 extremities (71-80%) and are largely non-contact in nature, with a high proportion of ligament sprains  
60 occurring at the ankle and knee (26, 39). Deficits in neuromuscular control and aberrant movement  
61 patterns such as cutting, turning, and landing occurring frequently during game activities, (Price et al.,  
62 2004) are suggested pathomechanics (1, 47) that underlie sport-related injury (16).

63 Assessments of neuromuscular control have been analyzed previously in adults and female  
64 athletes including a predominance of jump-landing tasks using force plate diagnostics (18, 33, 34, 36,  
65 45). In order to accurately assess neuromuscular control in male youth soccer players, there is a need  
66 for reliable and valid testing protocols (41). Currently in youth males, the most common mode of  
67 assessment is measurement of landing forces during a drop vertical jump (DVJ) (24, 25, 40). This  
68 protocol has shown strong reliability in male and female high school athletes (ICC range = 0.89 – 0.98)  
69 (40). However, single leg horizontal and vertical jumps should also be considered due to the type and  
70 frequency of related movements during game play. Strong test re-test reliability has also been reported  
71 for measures of concentric peak force and power during a single leg vertical jump (ICC range = 0.88 –  
72 0.97) in healthy teenagers (5). Available data in male youth soccer players and assessments of landing  
73 force are sparse.

74 In addition to the quantification of landing forces, measurement of dynamic stability may also  
75 provide useful information. “Time to stabilization” (TTS) calculations report deficits in postural control  
76 and reflex stabilization in subjects with functional ankle instability (44) and anterior cruciate ligament  
77 (ACL) deficiency (50). TTS is the speed in which individuals stabilize within a pre-determined ground  
78 reaction force range upon landing (11, 45). Although TTS has been quantified from a variety of jump-  
79 landing tasks (11), the most common method is a single leg horizontal hop onto a force plate (3, 33,  
80 43). Limited data is available in youth athletes, however, ground reaction force measures in adults

81 during single leg horizontal hops appear to be more reliable than centre of pressure values (ICC range  
82 = 0.87-0.97 vs. 0.53-0.75) (6, 45). Strong within-session reliability has also been reported for both  
83 dominant ( $r = 0.82$ ) and non-dominant ( $r = 0.87$ ) limbs (33).

84 In spite of this growing body of evidence, kinetic landing assessments have been utilized less  
85 often in paediatric male athletes. Poor attenuation of ground reaction forces during landing tasks may  
86 increase the risk of lower extremity injury (27). Practitioners utilizing such assessments for pre-  
87 participation screening require a greater understanding of their accuracy in this cohort. Previous  
88 research investigating the effects of age, growth and maturation on jumping tasks has shown a trend of  
89 increased performances with age (12, 37). However, variation across growth and maturation may also  
90 be evident (28, 37) and movement variability during jumping tasks is more evident in younger athletes  
91 (16). To the author's knowledge, no data currently exists to confirm the reliability of jump-landing  
92 kinetic assessments for male youth soccer players. This paucity of literature does not permit accurate  
93 interpretation of results following intervention or deficit assessments relative to the typical error.  
94 Research is also required to examine the effects of maturation on these measures due to the likelihood  
95 of greater movement variability in younger players. Therefore, the aim of this study is to determine the  
96 within-subject reliability of a field-based neuromuscular control screening battery using force plate  
97 diagnostics in elite male youth soccer players at different stages of growth and maturation.

98

## 99 **METHODS**

### 100 *Experimental Approach to the Problem*

101 This study used a repeated measures design to determine the intersession reliability of a range of field-  
102 based neuromuscular control assessments. Participants were required to attend the club training ground  
103 on three occasions separated by a period of seven days. The first session was used to familiarize subjects  
104 with the test equipment and assessment protocols. In the second and third sessions, data was collected  
105 to determine test-retest within-subject variation for the reliability study. Three different force plate  
106 diagnostic assessment protocols were used, including: a drop vertical jump (DVJ), a single leg 75%

107 horizontal hop and stick (75%HOP) and a single leg countermovement jump (SLCMJ). A 10-minute  
108 standardized dynamic warm up was completed prior to each session. The order of testing was  
109 randomized using a counterbalanced design to reduce the potential for an order effect. This  
110 randomization process was also applied for all unilateral jumps to determine the order of which leg was  
111 tested first. For the purposes of data collection, three trials were analyzed and one minute of recovery  
112 was allowed between trials based on previous recommendations (11). Testing was completed at the  
113 same time on each day, and participants were asked to wear the same training kit and footwear, and  
114 refrain from strenuous exercise at least 48 hours prior to testing. Subjects were also asked to eat  
115 according to their normal diet and avoid eating and drinking substances other than water one hour prior  
116 to each test session.

117

### 118 *Subjects*

119 Participants were grouped as either pre- or post-peak height velocity (PHV) which has been defined as  
120 the maximal rate of growth during the adolescent growth spurt (29). This group separation was applied  
121 to examine if a players stage of maturation affects the reliability of the test measures included in this  
122 study due to previous research indicating greater movement variability is present in younger children  
123 (15). Twenty five pre-PHV (age  $11.93 \pm 0.43$  yr; height  $151.40 \pm 4.84$  cm; body mass  $41.05 \pm 5.62$  kg;  
124 maturity offset  $-2.34 \pm 0.41$  yr) and twenty five post-PHV (age  $17.26 \pm 0.69$ ; height  $178.22 \pm 5.47$ ;  
125 body mass  $72.27 \pm 6.93$  kg; maturity offset  $2.91 \pm 0.81$  yr) youth soccer players from the academy of a  
126 professional English Championship soccer club volunteered to take part in the study.. Subjects were  
127 familiar with regular performance evaluations and none of the players reported injuries at the time of  
128 testing. Parental consent, participant assent and physical activity readiness questionnaires were  
129 collected prior to the commencement of testing. Ethical approval was granted by the institutional ethics  
130 committee in accordance with the declaration of Helsinki.

131

### 132 *Procedures*

133 *Anthropometry*

134 Body mass (kg) was measured on a calibrated physician scale (Seca 786 Culta, Milan, Italy). Standing  
135 and sitting height (cm) were recorded on a measurement platform (Seca 274, Milan, Italy). Seated height  
136 was measured with subjects sat on a box and their back against an upright stadiometer. The height of  
137 the box was then subtracted to provide the recorded value. Using anthropometric measures (age, body  
138 mass, standing height and sitting height, biological maturation was measured utilising the regression  
139 equation of Mirwald et al. (32). The equation has previously been validated for boys with a standard  
140 error of estimate of 0.57 years (Mirwald et al., 32).

141

142 *Drop Vertical Jump (DVJ)*

143 Participants were positioned on top of a box at a height of 30 cm. Instructions were to drop directly  
144 down with no vertical elevation onto two separate force plates (Pasco, Roseville, California, USA)  
145 positioned 8 cm apart. Upon ground contact, players immediately performed a maximum vertical jump  
146 aiming to jump as high as possible and then land on the plates and stick the landing as per previous  
147 guidelines (34). Hands were freely available to replicate a natural jump-landing position (34, 40). Only  
148 the data from the first landing was used for subsequent analysis.

149

150 *Single leg 75% Horizontal Hop and Stick (75%HOP)*

151 A tape measure was marked out to a three metre distance on a horizontal line with the zero cm mark  
152 positioned in line with the centre of a force plate (Pasco, Roseville, California, USA). Participants began  
153 by standing in line with the force plate on the designated test leg; hands on their hips and toe in line  
154 with a distance marker on the tape measure representing 75% of their predetermined maximal single  
155 leg hop and stick performance. Instructions were to hop forward onto the force plate, landing on the  
156 same leg with the hands remaining on their hips throughout. Players were required to stick the landing  
157 and hold for a period of five seconds, remaining as still as possible without any other body part touching  
158 the floor (11).

159

160 *Single Leg Counter Movement Jump (SLCMJ)*

161 Participants stood on a force plate (Pasco, Roseville, California, USA) in a unilateral stance with their  
162 hands on their hips and the opposite hip flexed at 90° to ensure minimal contributions from the  
163 contralateral leg. Instructions were to jump as high as possible using a countermovement by dropping  
164 to a self-selected depth and then immediately triple extending at the ankle, knee and hip in an explosive  
165 concentric action. On ground contact, subjects were required to stick the landing and hold for a period  
166 of five seconds remaining as still as possible. Bending of the knees whilst airborne was not permitted,  
167 and hands remained in contact with hips throughout the test (11).

168

169 *Force Plate Variables*

170 Kinetic landing data captured from the force platform included: peak vertical ground reaction force  
171 (pVGRF) recorded in the first 100ms following ground contact, time to pVGRF, and pVGRF  
172 asymmetry during for all tests. A cut-off point of 100ms was used to determine pVGRF due to the  
173 reported timing of non-contact injuries which occur within a similar time-frame following initial ground  
174 contact (22). Forces experienced after this point are unlikely to contribute to acute injury risk and were  
175 therefore not included in the analysis. In the SLCMJ and 75%HOP protocols, time-to-stabilisation  
176 (TTS) was also quantified from the vertical force vector. Vertical TTS was calculated as the time taken  
177 from ground contact to the first point when the vertical force component reached and stayed within 5%  
178 of body weight for a period of one second (11, 14). The point of ground contact was then subtracted  
179 from this value in accordance with previous guidelines (11). For the DVJ and 75%HOP protocols, initial  
180 contact was defined as the point when vertical ground reaction force first exceeded 10 N. In the SLCMJ,  
181 the same criteria were used to determine initial contact following the preceding propulsive and flight  
182 phases. All data were recorded at a sampling rate of 1000 Hz and filtered through a fourth-order  
183 Butterworth filter. A cut-off frequency of 18, 21, and 26 Hz was used for the SLCMJ, DVJ, and  
184 75%HOP respectively.

185

186 *Asymmetry Calculation*

187 To quantify asymmetry, the percentage difference between the highest and lowest performing limb was  
188 used. The value obtained is expressed as the absolute percentage of performance achieved using the  
189 higher performing limb as the reference (see equation 2).

190

191 
$$\text{Asymmetry \%} = \text{ABS}(\text{lowest performing limb} - \text{highest performing limb})$$

192 
$$/ \text{highest performing limb} * 100$$

193

194 
$$\% \text{ of Performance achieved} = 100 - \% \text{ Asymmetry}$$

195

[equation 2]

196

197 *Statistical Analysis*

198 The data was checked for normality and descriptive statistics for each test were calculated across the  
199 two testing sessions. To determine systematic bias between trials, a series of paired samples t-tests were  
200 used for all measures with a  $p$  value  $\leq 0.05$  indicative of a significant difference between the two trials.  
201 Within-subject variation was determined using mean coefficients of variation (CV %). Further  
202 reliability statistics included: change in mean and intra-class correlation coefficient (ICC). 95%  
203 confidence intervals (95% CI) were used and all reliability data was computed through Microsoft  
204 Excel<sup>®</sup> 2010 using a freely available spread sheet (20). Paired samples t-tests were processed using  
205 SPSS<sup>®</sup> (V.21. Chicago Illinois).

206



207 **RESULTS**

208 Descriptive statistics and all reliability measures calculated for each test are displayed in tables 1 and  
209 table 2 for pre- and post-PHV groups respectively. No significant differences were reported for the test  
210 variables when the mean scores of the two test trials were analyzed using a series of paired samples t-  
211 tests ( $P > 0.05$ ).

212

213 \*\*\*\*\* *Insert tables 1 and 2 near here* \*\*\*\*\*

214

215 Following the analysis of all variables, measures highlighted with acceptable CV values ( $\leq 10\%$ ) (8)  
216 were then further investigated to determine the reliability of lower-limb asymmetry (table 3). In both  
217 groups, all measures reported acceptable CV values ( $\leq 10\%$ ) with the exception of 75%HOP pVGRF in  
218 pre- (CV = 11.8%) and post-PHV (13.2% post-PHV) cohorts.

219

220 \*\*\*\*\* *Insert table 3 near here* \*\*\*\*\*

221

222 **DISCUSSION**

223 The current study assessed the reliability of a field-based neuromuscular control screening battery using  
224 force plate diagnostics in elite male youth soccer players who were either pre- or post-PHV. In both  
225 groups, pVGRF in the 75%HOP and SLCMJ demonstrated acceptable reliability ( $CV \leq 10\%$ ).  
226 However, greater variability was evident in the DVJ test as indicated by higher CV values. Irrespective  
227 of test protocol, variability was more pronounced in the pre-PHV group than the post-PHV cohort.  
228 Asymmetry values for the measures identified ( $CV \leq 10\%$ ) were also analyzed and reported largely  
229 acceptable reliability ( $CV \leq 10\%$ ). The within-subject variance of all other assessed variables, across  
230 all three protocols, exceeded the threshold for acceptable reliability ( $CV > 10\%$ ) in both groups.

231 In both groups, pVGRF was the most reliable kinetic measurement reflected by the lowest CV%.  
232 These findings are commensurate with Cordova et al. (7) who reported excellent reliability values (ICC  
233 = 0.94; SEM = 0.003% body weight) during a SLCMJ onto a force plate. Other studies have also  
234 reported high within-session reliability in adults for pVGRF during a single leg hop and stick (ICC =  
235 0.82 to 0.87) (3) and inter-session reliability of a single leg horizontal drop jump (CV = 5.71) (46).  
236 Conversely, vertical impulse (a measure comprised of both force and time) was shown to display greater  
237 test re-test variation (8.28%) (46). In the present study, while not a direct measure of impulse, time to  
238 pVGRF also showed higher CV values indicating greater within-subject variation for these metrics in  
239 male youth soccer players.

240 In this study, pVGRF in both the SLCMJ and 75%HOP tests demonstrated lower within-subject  
241 variation than the DVJ. In school children, strong reliability for measures of pVGRF force at landing  
242 (ICC = 0.89), and take-off (ICC = 0.98) has been reported (40). In the present study, lower reliability  
243 was displayed in the pre-PHV group which may be indicative of reduced skill levels, and immature pre-  
244 frontal motor cortex activation for cognitive control resulting in greater variation in the execution of  
245 motor control tasks (4). Additionally, increased jumping skill has been associated with an enhanced  
246 ability to absorb landing forces (38). As males progress through adolescence they appear to display an  
247 increased ability to attenuate landing forces, possibly due to the presence of the neuromuscular spurt  
248 (40). Conversely, younger children appear to land with greater knee and hip extension, which combined  
249 with heightened muscle co-contraction upon impact, will lead to higher pVGRF (9, 48). Supporting this  
250 notion, lower pVGRF related to body mass during the breaking phase of a DVJ have been reported in  
251 adults versus boys (25). This may be due to more efficient stretch reflex utilization and greater levels  
252 of muscle activation prior to landing and during the breaking phase of the jump (24). Data also shows  
253 that as children mature they become more reliant on supra-spinal feed forward input and short latency  
254 stretch reflexes (28). Cumulatively, the combination of movement inefficiency and higher landing  
255 forces may provide a rationale for the greater variability in pVGRF within the pre-PHV soccer players  
256 in this study.

257 During the 75%HOP and SLCMJ, high CV's were reported for TTS in both groups. These values  
258 indicate large within-subject variance and thus, caution should be applied when using this measurement  
259 in male youth soccer players. Obtaining high reliability for repeated trials during tasks requiring  
260 dynamic postural stability is difficult (11). Single leg jumping and landing activities that rely on  
261 reflexive muscle responses, proprioceptive and kinaesthetic feedback will typically utilise a range of  
262 movement strategies and therefore increase variability (11, 51). No data is available to compare the  
263 results of this study to those of similar populations, however, reliability statistics in adults suggest strong  
264 test re-test comparisons in single leg hop tasks ( $ICC = 0.87 - 0.97$ ) (6, 45). A plausible explanation for  
265 the high CV% in this study in comparison to adult data could be age-related factors, such as, growth,  
266 maturation and skill. Previous literature has suggested that maturation of the neurological, visual,  
267 vestibular and proprioceptive systems may lead to enhanced performance during single leg balancing  
268 tasks (31). Also, younger subjects demonstrate greater postural sway during single leg balance  
269 manoeuvres which may compromise stability (31). Thus, measures of reflex stabilization may be  
270 subject to greater variability in male youth soccer players.

271 Task demands are another factor which may explain the differences in reported reliability from  
272 this study and those of previous investigations. In the present study, two single leg landing assessments  
273 were used to provide data for both horizontal and vertical jumping tasks. Conversely, the  
274 aforementioned studies used horizontal tasks only and a standardised distance from the force plate of  
275 either leg length (6), or an arbitrary distance of 70 cm (45). The utilization of anthropometric measures  
276 or standardised distances may subsequently over or under-estimate an individual's performance. For  
277 example, an athlete with short legs may demonstrate a reduced TTS due to the relatively shorter hopping  
278 distance required. However, during a maximal single leg hopping task, the same athlete may be capable  
279 of much greater jump distances than that of their leg length. These abilities are likely to be replicated  
280 under conditions of competitive soccer match play; thus, an individual's inherent risk of injury is likely  
281 a product of how far they can jump and how well they can attenuate the resultant forces upon landing.

282 The methods of calculating TTS could also account for inconsistencies with the available  
283 literature. In the current study, TTS was measured based on previous recommendations (11, 14).

284 Conversely, Colby et al. (6) and Ross et al. (45) used both anterior-posterior and medio-lateral force  
285 vectors and a static hold of twenty seconds, scanning the components from the last two windows of the  
286 last 10s (i.e. at 10-15s and 15-20s), and the smallest ground reaction force range was accepted as the  
287 optimal range variation (43). This method, while displaying sound reliability, raises concerns of  
288 ecological validity when screening male youth soccer players. For example, if young soccer players are  
289 required to spend up to 20 seconds standing still on a force plate, they are likely to demonstrate greater  
290 postural sway, thus affecting their ground reaction force range. The shorter recording period of five  
291 seconds used in this study as opposed to 20 seconds (43) also has implications for testing a large number  
292 of athletes, particularly youth athletes who may demonstrate lower levels of concentration.

293         Despite their frequency of use, limited data is available to report the reliability of limb asymmetry  
294 statistics during unilateral jumping tasks. One available study in ACL patients determined the ‘limb  
295 symmetry index’ for a range of hopping based tests using ICC and standard error of measurement (ICC  
296 = 0.82 – 0.93; SEM = 3.04 – 5.09) (42). The authors assessed differences between the injured and non-  
297 injured leg, whereas, previous research has analyzed the difference between the dominant and non-  
298 dominant legs although no reliability data was reported (2, 30). In high school male and female soccer  
299 players, strong reliability of force production and attenuation measures has been shown (ICC > 0.97),  
300 however, specific outcome measures were not reported (17). The present study showed acceptable  
301 reliability values for most of the measures included and calculated asymmetry using the highest versus  
302 lowest performing leg. This accounts for neuromuscular inhibition which can occur following an injury  
303 to a specific limb (13, 35) and the requirement to jump and land repeatedly on both legs during a soccer  
304 competition. No data is available in youth male soccer players to compare the findings of this study;  
305 further investigations are needed to examine the reliability of asymmetry values using the  
306 aforementioned methods during a variety of jump-landing tasks.

307         A number of the variables measured in this study demonstrated low ICC statistics. It has been  
308 suggested previously that an ICC value > 0.75 is acceptable and values below this provide inadequate  
309 reliability (23). However, re-test correlations measure how closely the values of two trials track each  
310 other specific to each individual and the reproducibility of the rank order of subjects during the re-test

311 (19). Low values indicate that subjects did not retain their order during the re-test. Furthermore, a  
312 homogenous sample will also likely demonstrate a low value (19). The subjects in this study are  
313 reflective of a homogenous sample and this provides a plausible explanation for lower ICC values than  
314 those in other studies. Specifically, a number of the test variables in this study reported lower ICC  
315 values in the pre-PHV players. Due to their status as prepubescent athletes, performance levels may be  
316 more clustered as they have not yet experienced their peak growth spurt; the possibility of players  
317 changing their rank order is high. The post-PHV players were likely at different stages of physical  
318 development with some players further past the period of PHV than others; changing of rank order may  
319 be less frequent, as evidenced by predominantly higher ICC values.

320

## 321 **PRACTICAL APPLICATIONS**

322 Reliability data is now available for a field-based battery of neuromuscular control assessments using  
323 force plate diagnostics to screen male youth soccer players for potential injury risk. Practitioners can  
324 benefit from this data by selecting from the wide range of assessments available in the literature by  
325 considering their reproducibility as a basis for test re-test comparison. Furthermore, using the reliability  
326 statistics derived from this study, the smallest worthwhile change can be determined by calculating the  
327 between-subject standard deviation for each test and multiplying this number by 0.2 or 0.5% of the CV  
328 (21). If this value is within the error range (CV %) reported by the test, then it can be deemed reliable  
329 for use (49). Also, coaches applying interventions to reduce injury risk can accurately establish if the  
330 measured effects are reflective of a true change in performance.

331         Acceptable reliability values were reported for a variety of measures. In both the pre and post-  
332 PHV groups, pVGRF in both the 75%HOP, and SLCMJ demonstrated acceptable reliability (CV  $\leq$   
333 10%). These variables should be considered reliable for assessing elite male youth soccer players.  
334 However, greater within-subject variation was evident during the DVJ for all recorded variables; thus,  
335 caution should be applied when utilizing these protocols in this cohort. Overall, the results of this study  
336 suggest that pVGRF and asymmetry can be reliably assessed using a 75%HOP and SLCMJ in male

337 youth soccer players. These measures could realistically be utilized to support a screening battery for  
338 elite male youth soccer players and for test re-test comparison. Future research should examine if these  
339 measures can discriminate between injured and non-injured soccer players to determine their sensitivity  
340 in prospectively predicting injury risk.

341

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