

1 Article

2 Effect of hydroxyapatite nanoparticles on the 3 degradability of of random poly (butylene 4 terephthalate-co-aliphatic dicarboxylate)s having a 5 high content of terephthalic units

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16 **Abstract:** Copolyesters derived from 1,4-butanediol and constituted also by aliphatic and
17 aromatic dicarboxylate units in a molar ratio of 3:7 were synthesized by a two-step
18 polycondensation procedure. Succinic, adipic and sebacic acids were specifically selected as the
19 aliphatic component whereas terephthalic acid was chosen as the aromatic moiety. The second
20 synthesis step was a thermal transesterification between the corresponding homopolymers, being
21 always attained a random distribution as verified by NMR spectroscopy. Hybrid polymer
22 composites containing 2.5 wt-% of hydroxyapatite (HAp) were also prepared by *in*
23 *situ* polymerization. Hydroxyl groups on the nanoparticle surface allowed the grafting of polymer
24 chains in a way that composites were mostly insoluble in the typical solvents of the parent
25 copolyesters.

26 HAp had some influence on crystallization from the melt, thermal stability and mechanical
27 properties. HAp also improved the biocompatibility of samples due to the presence of Ca⁺² cations
28 and the damping effect of phosphate groups.

29 Interestingly, HAp resulted in a significant increase in the hydrophilicity of samples, which
30 considerably affected both enzymatic and hydrolytic degradability. Slight differences were also
31 found in the function of the dicarboxylic component, as the lowest degradation rates was found for
32 the sample constituted by the most hydrophobic sebacic acid units.

33 **Keywords:** poly(butylene terephthalate); copolyesters; hydroxyapatite; nanocomposites;
34 biocompatibility; hydrolytic degradation; enzymatic degradation

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36 1. Introduction

37 Polyesters are currently among the most competitive biodegradable polymers commercialized
38 as both commodity and speciality products. Applications range from materials for solving “white
39 pollutions concerns” caused by non-degradable polymers to materials with good properties to fulfil
40 for example the highly restrictive requirements in biomedical field [1-3]. The most common
41 polyesters are prepared by ring opening polymerization of lactones (e.g., polyglycolide, polylactide

42 and poly(ϵ -caprolactone) [4-5], but the production of poly(alkylene dicarboxylate)s has attracted a
43 great deal as well, especially for commodity applications [6].

44 Poly(butylene succinate) (PBS) is considered as one of the most important biodegradable
45 poly(alkylene dicarboxylate)s commercialized up to now, because of its considerable combination of
46 desired properties (e.g. high biodegradation rate, elastic modulus and melting point) [7,8]. Such
47 features generally worsen when another diol or aliphatic dicarboxylic acid is employed, making it
48 very interesting to incorporate rigid units such as aromatic dicarboxylates to avoid any
49 performance drop. Polyesters derived from aromatic dicarboxylic acids are much less electrophilic
50 and, thus, far less sensitive to hydrolysis than aliphatic polyesters. However, aromatic polyesters
51 may possess higher melting temperature (T_m 's) and better mechanical properties. Therefore, it is an
52 attractive challenge to incorporate aliphatic units randomly and determine if it is possible to
53 optimize the properties in the direction of a satisfactory rate of biodegradation while retaining good
54 mechanical properties. In the range of 30 mol% to 60 mol% of terephthalic acid, which is of particular
55 interest since such materials provide useful material properties, the degradation rate drops linearly
56 with the content of the aromatic acid [9,10]. Furthermore, these units may reduce the final cost of the
57 polymer. Therefore, BASF and Novamont have commercialized aliphatic-aromatic polyesters
58 derived from 1,4-butanediol and either adipic and terephthalic acids (i.e. Ecoflex™ and Origo-Bi™,
59 respectively).

60 Biodegradation of these polymers by microorganisms or in a compost site is well-proved, with
61 the degradation process being promoted by a lipase-like hydrolase enzyme [11-14].

62 Biodegradation rate of aliphatic-aromatic polyesters depends on different interplaying factors
63 such as: a) chain microstructure (e.g. random or blocky disposition), b) aromatic content and c) the
64 degree of crystallinity [15-21]. For example, note that a comonomer content close to 50% and a
65 random microstructure is expected to result in a decrease in the degree of crystallinity and logically
66 an increase in the degradation rate.

67 The present work has been focused on aliphatic-aromatic polyesters derived from 1,
68 4-butanediol, different aliphatic dicarboxylic acids (i.e. succinic, adipic and sebacic acids) and a high
69 content of terephthalic acid (i.e. a nominal value of 70 molar-% with respect to the total dicarboxylic
70 acid content was selected in order to explore the possibility to maintain the biodegradable
71 characteristics at such high content). In this case, one should expect a low degradation rate as a result
72 of such high aromatic content and the relatively high degree of crystallinity. Incorporation of
73 hydrophilic hydroxyapatite (HAp) nanoparticles may increase both biodegradability and
74 biocompatibility, and can be considered as an interesting option which will be evaluated for the new
75 proposed copolymers. To this end, copolymers with a 2.5 wt-% of HAp will be synthesized as well.

76 HAp ($\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2$) is a bioceramic which forms part of the majority of the inorganic
77 components of hard and connective tissues such as bones, teeth and tendons. Nowadays,
78 development of HAp-based nanocomposites and biodegradable polymers are attracting an
79 increasing interest since the presence of hydroxyl groups in the added nanoparticles may enhance
80 polymer degradation. Furthermore, HAp particles can provide osteoconductivity and
81 osteo-gravitativity as well as improved mechanical properties [22].

82 Hybrid HAp/biodegradable polymer composites can be prepared by different techniques, such
83 as hot press molding, plasma spraying, solution compounding and also *in situ* polymerization which
84 is the most frequently employed method [23]. Distribution of nano-HAp particles in the organic
85 matrix and final mechanical properties of the composite mainly depend on the interface
86 compatibility between organic and inorganic phases. A good adhesion is expected when the hybrid
87 is prepared by *in situ* polymerization, taking the capability of hydroxyl groups of the HAp surface to
88 bind carboxyl groups of the growing poly(alkylene dicarboxylate) into account. Nevertheless, some
89 limitations may also be expected as a consequence of the low concentration and reactivity of
90 hydroxyl groups on the nanoparticle surface that could lead to a reduced number of grafted
91 molecules.

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94 2. Experimental Section

95 **Materials:** Terephthalic acid (TA) was supplied by Shahid Toundgoyan Petrochemical
96 Complex (Mahshar, Iran). Nanohydroxiapatite (n-HAp) was purchased from Beijing DK nano
97 technology Co., Ltd, China. 1,4-butanediol (BDO), sebacic acid (SeA), adipic acid (AdA) and succinic
98 acid (SuA) were brought from Daejung Chemical & Metal Co., Ltd, Korea. Titanium butoxide (TBT)
99 as polycondensation catalyst was purchased from Merck Co., (Darmstadt, Germany).

100 African green monkey kidney fibroblast-like (COS-7) and epithelial-like Madin-Darby Canine
101 Kidney (MDCK) cells (ATCC, USA) were used in this work. Fetal bovine serum (FBS) was
102 purchased from Gibco (Thermo Fisher Scientific Inc., Spain). Lipases from pancreas porcine and
103 *Pseudomonas cepacia* were purchased from Sigma Aldrich.

104 **Polymerization:** Synthesis of the three selected copolymers named as polybutylene
105 succinate-*co*-terephthalate (PBST), poly(butylene adipate-*co*-terephthalate) (PBA_dT) and
106 poly(butylene sebacate-*co*-terephthalate) (PBSeT) was performed in a home-made 1 L high pressure
107 reactor with effective stirring, following a two-step melt polycondensation procedure:

108 a) Synthesis of prepolymers from 1,4-butanediol and the selected dicarboxylic unit.
109 Polycondensation reactions were carried out using an excess of 1,4-butanediol (BDO) (i.e. 1.7:1
110 [OH]:[COOH]). After loading the reactor with 650 g of a mixture of BDO and the appropriate
111 dicarboxylic acid, the reaction mixture was firstly stirred for 30 min at 140 °C under a pressure of
112 3-3.5 bars. A flow of N₂ was provided to keep the required pressure while an electric condenser
113 allowed separating the condensed water and the excess of alcohol. Reaction temperature was then
114 increased to 215 °C, 207 °C, 200 °C and 220 °C, for sebacic, adipic, succinic and terephthalic acid
115 derivatives, respectively. The reaction was stopped when no more water could be recovered
116 (approximately after 180 min). In fact, the reaction extent could be evaluated by weighting the water
117 that was recovered at regular time intervals.

118 b) Vacuum polycondensation and thermal transesterification between aliphatic and aromatic
119 prepolymers. The appropriate mixtures constituted by a 0.3:0.7 molar ratio of prepolymers derived
120 from the aliphatic and aromatic acids and TBT as catalyst (1.4 mmol for 1 mol of dicarboxylic acid)
121 were transferred to the reactor for 10 min at 200 °C and atmospheric pressure. Temperature was
122 subsequently increased up to 250 °C while vacuum (of 20 mbar) was applied. Once the mixer torque
123 reached the desired value, the reaction was stopped (approximately after 150 min). Copolymers
124 were dissolved in 1,1,1,3,3,3-hexafluoroisopropanol (HFIP), precipitated in water, washed several
125 times with water, methanol and ether and finally dried in a vacuum desiccator.

126 The chosen procedure differs from the conventional syntheses based on thermal
127 polycondensation processes from an appropriate ratio of comonomers. The advantage of the
128 proposed synthesis is that copolymers with different composition (i.e. having different comonomer
129 ratios) can be easily obtained if desired from the corresponding homopolymers. Nevertheless, time
130 and reaction temperature of the second step appear highly important to achieve a random
131 microstructure that should be checked.

132 Nanocomposites were synthesized based on the same protocol, except for the addition of a 2.5
133 wt-% n-HAp at the beginning of copolymerization step. Nanocomposites will be referred to as
134 PBST-HAp, PBA_dT-HAp and PBSeT-HAp depending on the aliphatic dicarboxylic unit.

135 **Measurements:** Molecular weights were estimated by size exclusion chromatography (GPC)
136 using a liquid chromatograph (Shimadzu, model LC-8A) equipped with an Empower computer
137 program (Waters). A PL HFIP gel column (Polymer Lab) and a refractive index detector (Shimadzu
138 RID-10A) were employed. The polymer was dissolved and eluted in HFIP containing CF₃COONa
139 (0.05 M) at a flow rate of 1 mL/min (injected volume 100 µL, sample concentration 2.0 mg/mL). The
140 number and weight average molecular weights were calculated using polymethyl methacrylate
141 standards.

142 Carboxylic acid end-group content was calculated, 1 g of polymer was dissolved in 20 mL
143 chloroform and titrated using 0.05N KOH in methanol with red phenol as the indicator. The
144 carboxylic acid content [COOH] in meq/kg was measured using the following equation:

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$$[COOH] = \frac{(v - v_0) \times m \times 1000}{w} \quad (1)$$

147 Where v and v_0 are volume of the titrant (mL) for titration of the chloroform solution with and
148 without the analyte, respectively, m is titrant concentration (N), and w is weight (g) of the polymer
149 sample.

150 Infrared absorption spectra were recorded in the 4000-600 cm^{-1} range with a Fourier Transform
151 FTIR 4100 Jasco spectrometer dotted with a Specac model MKII Golden Gate attenuated total
152 reflection (ATR) cell.

153 $^1\text{H-NMR}$ spectra were acquired with a Bruker AMX-300 spectrometer operating at 300.1 MHz.
154 Chemical shifts were calibrated using tetramethylsilane as an internal standard. A mixture (1:1 v/v)
155 of deuterated chloroform and trifluoroacetic acid (TFA) was used as the solvent.

156 Calorimetric data were obtained by differential scanning calorimetry with a TA Instruments
157 Q100 series with T_{zero} technology equipped with a refrigerated cooling system (RCS). Experiments
158 were conducted under a flow of dry nitrogen with a sample weight of approximately 5 mg and
159 calibration was performed with indium. T_{zero} calibration required two experiments: the first
160 experiment was performed without any sample while in the second case sapphire disks were used.
161 A first heating run (20 $^\circ\text{C}/\text{min}$) was performed to determine melting temperature and enthalpy of the
162 as-synthesized sample. To erase the thermal history the sample was then kept in the melt state for
163 three minutes and subsequently cooled to room temperature (10 $^\circ\text{C}/\text{min}$) to obtain crystallization
164 data. Finally, a second heating run (20 $^\circ\text{C}/\text{min}$) was carried out to characterize the melt crystallized
165 sample.

166 Thermal degradation was studied at a heating rate of 10 $^\circ\text{C}/\text{min}$ with around 5 mg samples in a
167 Q50 thermogravimetric analyzer (TGA) of TA Instruments, under a flow of dry nitrogen. Test
168 temperatures ranged from 50 to 600 $^\circ\text{C}$.

169 A TA Instruments DMA Q800 was used to study the dynamic-mechanical properties of
170 materials. Prismatic rectangular samples (ca $10 \times 12 \times 1.3 \text{ mm}^3$) were analyzed in single-cantilever
171 mode at 1 Hz and 10 μm strain amplitude at 3 $^\circ\text{C}/\text{min}$ from -100 to 100 $^\circ\text{C}$.

172 Contact angles (CA) were measured at room temperature with sessile drops using an OCA-15
173 plus Contact Angle Microscope (Dataphysics, USA) and SCA20 software. Contact angle values of
174 the right and left sides of distilled water drops were measured and averaged. Measurements were
175 performed 10 s after the drop (0.5 μL) was deposited on the sample surface. All CA data were
176 obtained by averaging between six measurements on different surface locations.

177 Distribution of HAp nanoparticles in the composites was evaluated by means of a Philips
178 TECNAI 10 electron microscope at an accelerating voltage of 80 kV. Samples were prepared by
179 embedding the nanocomposite specimens. A low viscosity modified Spurr epoxy resin was
180 employed to embed the specimens before curing and cutting in small sections. In this case, Sorvall
181 Porter-Blum microtome equipped with a diamond knife was utilized. The thin sections were
182 collected in a trough filled with water and lifted onto carbon coated copper grids.

183 X-ray diffraction patterns were acquired using a Bruker D8 Advance model with Cu
184 $\text{K}\alpha$ radiation ($\lambda = 0.1542 \text{ nm}$) and the geometry of Bragg-Brentano, theta-2theta. A one-dimensional
185 Lynx Eye detector was employed.

186 Degradation studies: Thermally molded films were used for biocompatibility and degradation
187 studies. Briefly, polymers were heated up to 25 $^\circ\text{C}$ above their melting point for 2 min using a
188 hydraulic press equipped with heating plates and a temperature controller (Graseby Specac, Kent,
189 England). Pressure was progressively increased to 3-4 bars. Polymer films, with thickness of about
190 150 μm were recovered after cooling the mold to room temperature and subsequently cut to the
191 desired size.

192 Cell adhesion and proliferation assays: COS-7 and MDCK cells were cultured in Dulbecco's
193 modified Eagle medium (DMEM) as previously reported [24]. Square pieces ($10 \times 10 \times 0.15 \text{ mm}^3$) of
194 press molten films were placed and fixed in each well of a multiwell culture plate with a small drop
195 of silicone (Silbione[®] MED ADH 4300 RTV, Bluestar Silicones France SAS, Lyon, France). They were
196 then sterilized by UV-radiation in a laminar flux cabinet for 15 min. Thereafter, the samples were

197 stabilized for 24 h in 1 mL of medium under culture conditions. For cell adhesion and proliferation
 198 assays, aliquots of 50–100 μL containing 5×10^4 and 2×10^4 cells, respectively, were seeded onto the
 199 films in each well containing 1 mL of medium, and incubated for 24 h (adhesion assay) or 7 days
 200 (proliferation assay). Samples were evaluated by the standard adhesion and proliferation
 201 method [24]. The used procedure is based on a simple modification of the ISO10993-5:2009 standard
 202 test that describes the appropriate methodology to assess the *in vitro* cytotoxicity of medical devices.
 203 Finally, the cellular viability on materials was evaluated through the MTT assay [24]. The study was
 204 carried out using five replicates and the results were averaged. Samples with adhered and grown
 205 cells on the films were fixed with 2.5% *w/v* formaldehyde at 4 °C overnight. They were subsequently
 206 dehydrated and processed for observation via scanning electronic microscopy.

207 *In vitro* hydrolytic degradation assays were carried out in a pH 7.4 phosphate buffer (19.268 g of
 208 $\text{Na}_2\text{HPO}_4 \cdot 12\text{H}_2\text{O}$ and 1.796 g of KH_2PO_4 in 1L of deionized water) at 37 °C and at the accelerated
 209 condition provided by raising temperature to 70 °C. Samples (2×2 cm² square pieces) were kept
 210 under orbital shaking in bottles filled with 20 mL of the degradation medium and sodium azide
 211 (0.03 wt-%) to prevent microbial growth for the selected exposure times. The samples were then
 212 thoroughly rinsed with distilled water, dried to constant weight under vacuum and stored over
 213 P_4O_{10} before analysis. Degradation studies were performed in triplicate and the results were
 214 averaged.

215 Enzymatic studies were carried out with lipases from *porcine* pancreas (56–60 U/mg) and
 216 *Pseudomonas cepacia* (≥ 30 U/mg) using three replicates. All samples (1×1 cm² square pieces) were
 217 exposed to 2 mL of pH 7.4 phosphate buffer at 37 °C. The buffer contained the enzyme along with
 218 sodium azide (0.03% *w/v*) and calcium chloride (5 mM). Solutions were replaced every 48 h to
 219 prevent enzymatic activity loss. Samples were extracted, washed and dried as indicated before.

220 Scanning electron microscopy (SEM) was utilized to examine the morphology of films after
 221 different times of exposure to the selected degradation media. Carbon coating was accomplished
 222 with a Mitec k950 Sputter Coater (fitted with a film thickness monitor k150x). SEM micrographs
 223 were obtained with a JEOL JSM-6400 instrument.

224 Weight retention (W_r) of the specimens was addressed by the percentage ratio of weight after
 225 degradation (W_d) to initial weight before degradation (W_0):

$$W_r = W_d / W_0 \times 100 \quad (2)$$

226 3. Results and Discussion

227 3.1. Synthesis and characterization of copolymers and nanocomposites

228 All copolymers were obtained with a high yield that ranged between 85% and 90%, being not
 229 observed a specific trend concerning the length of the aliphatic copolymer or the incorporation of
 230 HAp nanoparticles. The carboxyl content was always below 50 meq, indicating that degradation during
 231 polymerization step was not significant despite the recovered solid had a slightly brown/gray appearance.
 232 Nevertheless, white products were obtained after purification. Weight average molecular weights of
 233 purified copolymers varied between 17,100 g/mol and 20,200 g/mol and the polydispersity index
 234 remained in the typical range of polycondensation samples (i.e. between 2.1 and 2.4) (Table 1).

235 **Table 1.** GPC molecular weight data and polymerization yields.

236	Copolymer	Yield (%)	COOH (meq/g)	M_n (g/mol)	M_w (g/mol)	PDI
237	PBST	89%	17	9,540	20,200	2.12
238	PBAAdT	85%	31	7,800	17,100	2.19
239	PBSeT	90%	25	7,000	17,100	2.44
	PBST-HAp	91%	15	9,500	23,100	2.43
	PBAAdT-HAp	88%	23	9,800	26,200	2.67
240	PBSeT-HAp	90%	23	9,000	22,000	2.44

241 Nanocomposites prepared by *in situ* polymerization were highly insoluble and a high
 242 proportion remained as whitish particle dispersion in the HFIP solvent used for GPC measurements
 243 (inset of Figure 1). This feature indicates a significant grafting as the consequence of reaction
 244 between hydroxyl groups on the HAp surface with terminal carboxylic groups of the growing
 245 copolymers. Nevertheless, a small fraction corresponding to the lower molecular weight chains (i.e.
 246 those that were practically ungrafted) could be dissolved in HFIP at a low concentration. In this case,
 247 M_w values ranged between 22,200 g/mol and 26,170 g/mol, with the molecular size being always
 248 greater than the size determined for the corresponding copolymers. The greatest difference was
 249 found in the case of the adipic derivative (i.e. from 17,070 g/mol to 26,170 g/mol) and in particular,
 250 GPC curves showed a peak broadening and shift for the nanocomposite (Figure 1) due to presence of
 251 some grafted chains. In fact, the polydispersity index of the three nanocomposites was always
 252 greater (i.e. 2.4–2.7 with respect to 2.1–2.4) than that determined for copolymers, indicating a wider
 253 size distribution which reflects the presence of a small ratio of cross-linked chains. Note that a lower
 254 molecular weight and a narrow distribution should be expected if only the smallest and non-grafted
 255 chains were dissolved.

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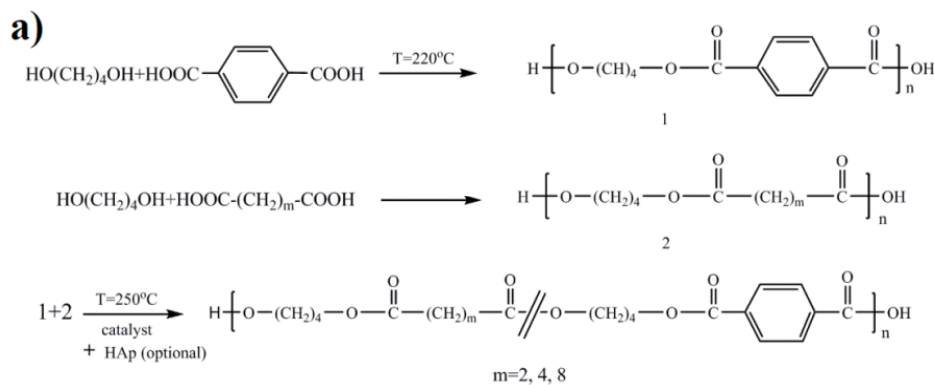
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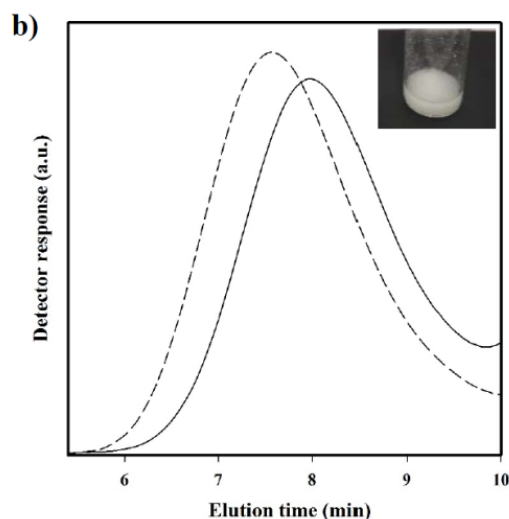
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Figure 1. a) Synthesis scheme for different studied copolyesters and nanocomposites. b) GPC curves of PBST (solid line) and PBST-HAp (dashed line) samples. The inset shows a photography of a high concentrated suspension of PBST-HAp in HFIP.

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FTIR spectra of copolymers and nanocomposites showed the characteristic absorption bands for methylene (2930 and 2850 cm^{-1} , stretching), $\text{C}=\text{O}$ (1701 cm^{-1} , stretching), aromatic $\text{C}-\text{O}$ (1284 and 1180 cm^{-1} , asymmetric and symmetric stretching, respectively), aliphatic $\text{C}-\text{O}$ (1220 and 1080 cm^{-1} , asymmetric and symmetric stretching, respectively), and aromatic (746 cm^{-1}) groups. A representative spectrum of PBTSu-HAp is illustrated in Figure 2. As the length of the aliphatic comonomer increased, the intensities associated with methylene groups were logically increased

277 compared to those related to the C=O group (inset of Figure 2). The bands corresponding to HAp
 278 could not be detected in the spectra of different composites due to the low loaded percentage of
 279 HAp.

280 ^1H NMR spectra were useful to determine the composition and to perform an analysis of
 281 sequences as previously reported for adipic acid copolymers [18]. Figure 3 shows the spectrum for
 282 the representative PBST copolymer. Table 2 summarizes the peak assignment for the three
 283 copolymers whereas the analyzed data are given in Table 3. The areas of signals at 8.14-8.17 ppm
 284 (terephthalate units, T) and 2.42-2.79 ppm (aliphatic dicarboxylate units, A) were used to determine
 285 the corresponding (f_T and f_A) mole fractions.

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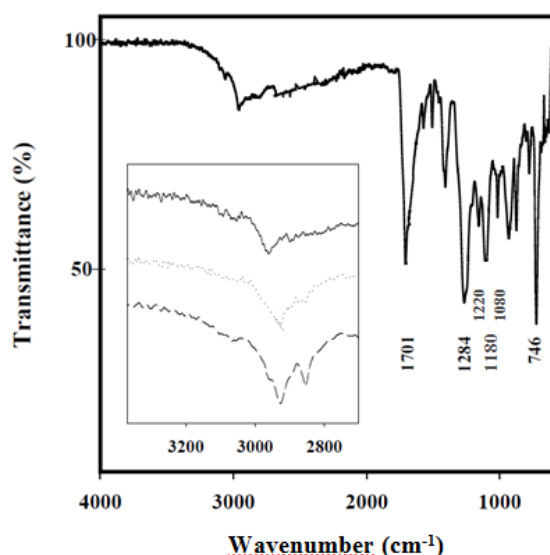
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Figure 2. FTIR spectrum of PBST-HAp. The inset compares the methylene bands of the three copolymers when spectra were normalized with the intensity of the C=O band.

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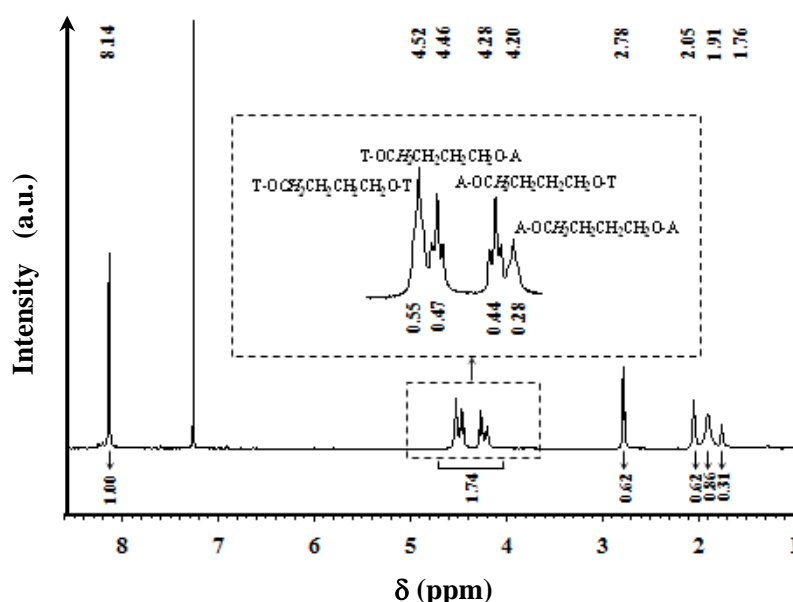
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Figure 3. ^1H NMR spectrum of PBST. The inset shows a magnification of the 4.70-4.25 ppm region where OCH_2 sequence sensitive signals appear.

317 The OCH_2 butanediol protons were highly sensitive to the neighbouring dicarboxylic acid units
 318 and consequently four multiplets were detected for all studied samples (Table 2).

319 The respective areas were used to determine the fractions corresponding to TBT (f_{TT}), TBA (f_{TA}),
 320 ABT (f_{AT}), and ABA (f_{AA}) sequences. Obviously f_{TA} and f_{AT} should be equal, being the summarized
 321 values averaged from the intensities of TCH₂..A and ACH₂...T signals. These values allowed
 322 determining the probability of finding a T unit next to an AB sequence (P_{AT}) as well as the
 323 probability of finding an aliphatic unit next to a TB sequence (P_{TA}):

$$324 \quad P_{AT} = f_{AT} / f_A \quad (3)$$

$$325 \quad P_{TA} = f_{TA} / f_A \quad (4)$$

326 Finally, block length of AB and TB sequences were calculated as:

$$327 \quad L_{rAB} = 1 / P_{AT} \quad (5)$$

$$328 \quad L_{rTB} = 1 / P_{TA} \quad (6)$$

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330 **Table 2.** Chemical shifts and assignments of the ¹H NMR spectra of synthesized copolyesters.

Sequence	Chemical Shift (ppm)		
	PBST	PBA _d T	PBSeT
-C ₆ H ₄	8.14	8.17	8.14
T-OCH ₂ CH ₂ CH ₂ CH ₂ O-T	4.52	4.57	4.64
T-OCH ₂ CH ₂ CH ₂ CH ₂ O-A	4.46	4.52	4.59
A-OCH ₂ CH ₂ CH ₂ CH ₂ O-T	4.28	4.31	4.37
A-OCH ₂ CH ₂ CH ₂ CH ₂ O-A	4.20	4.25	4.31
COCH ₂ -...	2.78	2.52	2.42
T-OCH ₂ CH ₂ CH ₂ CH ₂ O-T	2.05	2.08	2.06
T-OCH ₂ CH ₂ CH ₂ CH ₂ O-A	1.91	1.92	1.92
A-OCH ₂ CH ₂ CH ₂ CH ₂ O-A	1.76	1.80	1.79
COCH ₂ CH ₂ -...	-	1.72	1.64, 1.32

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332 The degree of randomness (r) is defined as the summation of the two
 333 probabilities (P_{AT} and P_{TA}), in which the values 2, 1 and lower than 1 are indicative of alternating,
 334 random, and blocky distributions. The limit value of 0 logically indicates a mixture of the two
 335 homopolymers. Values summarized in Table 3 indicate a composition close to the theoretical one,
 336 although copolymers were slightly impoverished on the aromatic units probably as a consequence
 337 of the lower molecular weight and the higher content in butanediol units of terephthalate
 338 prepolymers that caused a distortion in the calculation of theoretical feed ratio for the second
 339 synthesis step. Results also demonstrated that the three samples were associated with degree of
 340 randomness values close to 1.0, indicating a perfect statistical distribution. In fact, f_{TA} and f_{AT} values
 341 were consistent with those expected for a random distribution (e.g. 0.21 with respect to 0.22-0.25).
 342 Namely, transesterification reactions between prepolymers of each dicarboxylic acid should take
 343 place at high reaction temperature, hindering the possibility to achieve a blocky structure.

344 **Table 3.** Composition and sequence-distribution analysis of synthesized copolyesters.

Copolymer	Composition		Fraction of Diads Centered in the Butylene Units				Probability of Finding Units		Block Lengths		Degree of Randomness
	f_T	f_A	f_{TT}	f_{TA}	f_{AT}	f_{AA}	P_{TA}	P_{AT}	L_{rTB}	L_{rAB}	r
PBST	0.65	0.35	0.40	0.24	0.24	0.12	0.38	0.65	2.63	1.53	1.03
PBA _d T	0.64	0.36	0.38	0.25	0.25	0.12	0.39	0.61	2.56	1.64	1.00
PBSeT	0.65	0.35	0.45	0.22	0.22	0.11	0.34	0.70	2.94	1.43	1.04

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3.2. Thermal properties of copolyesters and nanocomposites

Figure 4 shows the typical protocol followed to determine the thermal properties of the synthesized samples taking PBAdT and PBAdTA-HAp as representative examples, whereas DSC data for all studied specimens are summarized in Table 4.

In all cases, the first heating run showed a complex melting behavior where two endothermic peaks appeared overlapped in practice. These melting temperatures were similar for all samples since fusion always corresponded to crystals predominantly constituted by butylene terephthalate sequences. Nevertheless, melting temperatures were clearly lower (i.e. by approximately 60 °C) than that reported for the PBT homopolymer (223 °C) [25]. Thus, a similar amount of aliphatic comonomer units seems to be incorporated into the crystals as could be expected by considering their similar composition (i.e. 30 molar-% of aliphatic dicarboxylic units). DSC scans suggest the occurrence during heating of a typical recrystallization process where thickening of lamellae took place, giving rise to a high temperature melting peak. Stability and thicknesses of lamellar crystals depend on the crystallization process. Thus, slight differences (i.e. peak temperatures and intensities) can be found between the first (i.e. solution crystallized sample) and the second heating (i.e. melt crystallized sample) runs as shown in Figure 4 for the PBAdT copolyester. Melting enthalpies of all samples were also similar, and no significant difference was observed when the aliphatic dicarboxylic acid was changed or HAp was incorporated. Random copolyesters had a moderate crystallinity as estimated from the composition and the melting enthalpy of 100% crystalline PBT (142 J/g) [26].

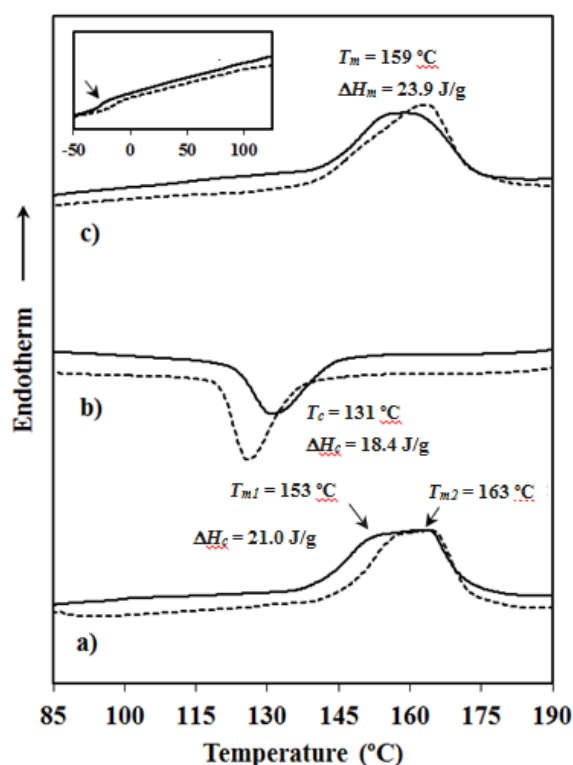


Figure 4. Typical sequence of DSC scans performed with PBAdT (solid lines) and PBAdT-HAp (dashed lines): a) The initial heating scan of the as-synthesized sample, b) The cooling run from the melt state, and c) The heating run of the melt crystallized sample. Calorimetric data are only given for the sample without HAp. Inset shows the low temperature region for (c) in which T_{gs} could be detected (arrow).

The effect of HAp was only remarkable in the case of the adipic acid derivative since in this case the glass transition temperature was significantly increased (i.e. from -27 °C to -14 °C) and the crystallization process required a higher supercooling, (Figure 4b) probably as a consequence of its

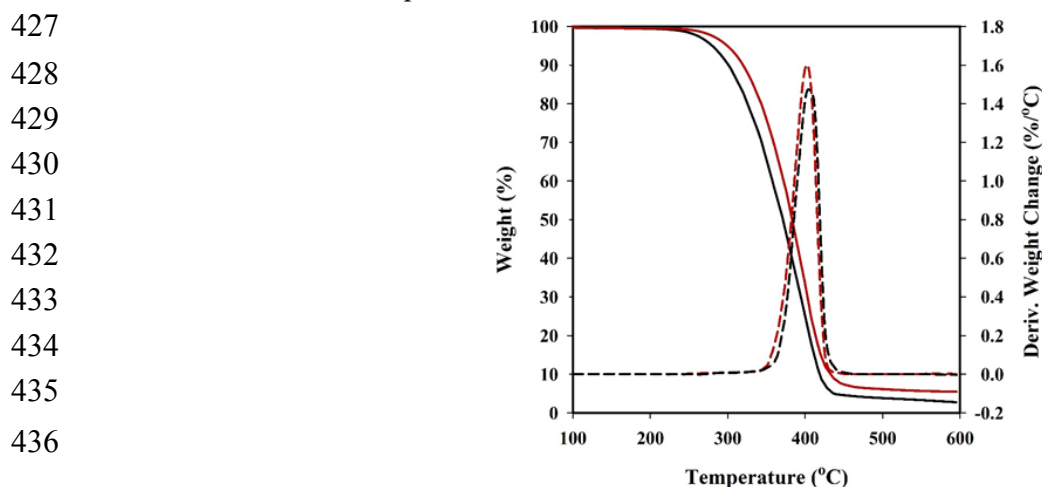
396 higher molecular weight. Crystallization of the nanocomposite rendered more defective or thinner
 397 lamellae as could be deduced by the decrease in both temperature and intensity of the first melting
 398 peak (Figure 4c). Namely, a recrystallization process during the second heating run was enhanced
 399 giving rise to a greater ratio of thicker lamellae and a higher intensity of the corresponding melting
 400 peak.

401 **Table 4.** Calorimetric data for the studied copolyesters and nanocomposites.

Sample	1 st Heating Run			Cooling Run			2 nd Heating Run		
	T_m (°C)	ΔH_f (J/g)	χ^a (%)	T_c (°C)	ΔH_c (J/g)	T_g (°C)	T_m (°C)	ΔH_f (J/g)	χ^a (%)
PBST	153, 159	19.6	21	119	15.9	-7	155, 159	20.8	22
PBAdT	153, 163	21.0	23	131	18.4	-27	159	23.9	26
PBSeT	159, 163	23.7	26	128	19.1	-27	164	20.6	22
PBST-HAp	149, 159	19.1	20	119	17.4	-7	158	21.9	23
PBAdT-HAp	158, 164	19.6	22	126	19.5	-14	163	23.8	26
PBSeT-HAp	160, 166	22.7	26	129	22.3	-27	162	23.4	27

410 ^a Degree of crystallinity of the aromatic phase estimated from the melting enthalpy reported for a
 411 100% crystalline PBT sample (ΔH^{100}) and the experimental composition determined by ¹H NMR (i.e.
 412 $\chi = \Delta H / (\Delta H^{100} \times m_T)$, m_T being the mass fraction of the BT repeat unit).

413 TGA and DTGA traces showed that all studied samples thermally degraded at a temperature
 414 clearly higher than the corresponding melting points. Although decomposition seems to proceed as
 415 a single step (e.g. Figure 5 for PBST), different mechanisms are probably involved as reported for
 416 PBT [27]. In this case, degradation started with an ionic decomposition process that results in the
 417 production of tetrahydrofuran. The subsequent process was associated with ester pyrolysis reactions
 418 that yield 1,3-butadiene at the beginning and finally produce aromatic species [27]. Thermal
 419 degradation of several poly(butylene succinate-co-butylene terephthalate)s has been also previously
 420 reported [28], indicating a single weight-loss step. Nevertheless, it was found that the aliphatic
 421 poly(butylene succinate) exhibited lower degradation temperature and thermal stability compared
 422 to PBT. The differences between our results and the previously reported data on the copolymer
 423 could be attributed to distinct chain microstructures due to alterations in the copolymerization
 424 process. Therefore in this study, the high temperature step was performed with a prepolymer
 425 mixture instead of a monomer mixture. Data summarized in Table 5 indicate a similar degradation
 426 behavior for succinic, adipic and sebacic acid derivatives.



437 **Figure 5.** TGA (solid lines) and DTGA (dashed lines) curves comparing the thermal degradation of
 438 PBST (black lines) and PBST-HAp (red lines) samples.

439 Curves for nanocomposites progressed in a similar way but the incorporation of HAp had two
 440 main effects: a) The DTGA peak associated with the first decomposition step was shifted by
 441 approximately 3 °C to higher temperatures. The observed stabilization may be a consequence of the
 442 reduction of free carboxylic groups due to the grafting reaction with the hydroxyl groups of HAp
 443 surface or even a hindered diffusion of degradation products. b) The char yield logically increased to
 444 a value that was fully consistent with the theoretical amount of incorporated HAp (e.g. from 2.8% to
 445 5.6% for the succinic derivative).

446 **Table 5.** TGA and DTGA data for thermal decomposition of the studied copolyesters and
 447 nanocomposites.

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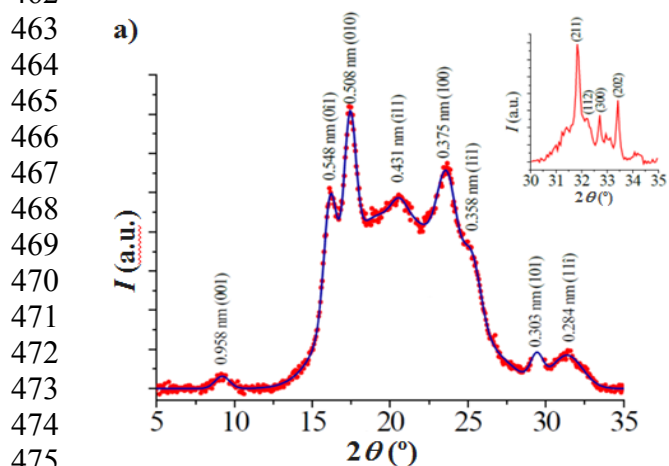
Sample	T_{onset} (°C)	T_{peak} (°C)	Char yield (%)
PBST	315	402	2.8
PBAdT	318	405	5.6
PBSeT	322	405	5.2
PBST-HAp	352	405	5.6
PBAdT-HAp	342	404	7.9
PBSeT-HAp	348	407	6.3

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450 3.3. X-ray diffraction data

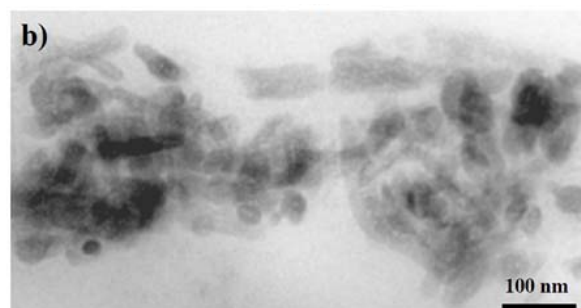
451 Powder X-ray diffraction patterns of all synthesized samples were similar and logically related
 452 to the structure of poly(butylene terephthalate). In particular, strong (001), (0-11), (010), (1-11), (100),
 453 (1-11), (101) and (11-1) reflections of the α -form defined by a triclinic unit cell ($a = 0.483$ nm, $b = 0.596$
 454 nm, $c = 1.162$ nm, $\alpha = 99.9^\circ$, $\beta = 115.2^\circ$, and $\gamma = 113.8^\circ$) and a gauche-trans-gauche conformation for the
 455 glycol unit were observed (Figure 6) [29, 30]. It is clear that copolymers crystallized according to the
 456 structure of the major component and that aliphatic comonomers should be mainly excluded from the
 457 crystalline phase, being probably located in the amorphous lamellar folds. Logically, the slight
 458 increase on the length of the aliphatic dicarboxylic unit should have a minor impact on the
 459 molecular arrangement of the crystalline phase. Patterns of nanocomposites also showed very low
 460 signals corresponding to HAp (inset of Figure 6a) related to the (211), (112), (300) and (202)
 461 reflections.

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Figure 6. a) X-ray diffraction profile of PBSTS-HAp with indication of the spacings of main reflections. The inset shows a magnification of the 2θ region between 30° and 35° where strongest reflections of HAp appear. b) Transmission electron micrograph of a thin section of PBTSu-HAp.

479 Transmission electron micrographs of nanocomposite thin sections revealed a relatively good
 480 dispersion of HAp thin crystals (Figure 6b). They showed a typical elongated hexagonal
 481 morphology with dimensions (length \times width) ranging from $100\ \mu\text{m} \times 50\ \mu\text{m}$ to $50\ \mu\text{m} \times 20\ \mu\text{m}$.

482 3.4. Mechanical properties

483 The effect of HAp particles on mechanical properties was evaluated by DMTA, and the main
 484 results are summarized in Table 6. Storage modulus (E') and loss tangent curves for representative
 485 PBAAdT and PBAAdT-HAp samples are shown in Figure 7. Some specific features that can be pointed
 486 out are as followings: a) Storage moduli of nanocomposites are always greater than those measured
 487 for parent copolyesters (e.g. $2470\ \text{N/m}^2$ with respect to $1840\ \text{N/m}^2$ at $-20\ ^\circ\text{C}$ and $700\ \text{N/m}^2$ with respect
 488 to $550\ \text{N/m}^2$ at $20\ ^\circ\text{C}$ for the adipic acid derivative). b) The intensity of the loss tangent peak decreases
 489 for the nanocomposite indicating a more restricted chain mobility, which cannot also be justified by
 490 the slight increase in crystallinity. c) Loss tangent curves show a predominant peak at a temperature
 491 close to $0\ ^\circ\text{C}$. This glass transition temperature only increased for the nanocomposite of the adipic
 492 acid and sebacic acid derivatives, with a very small observed variation (i.e. less than $5\ ^\circ\text{C}$).

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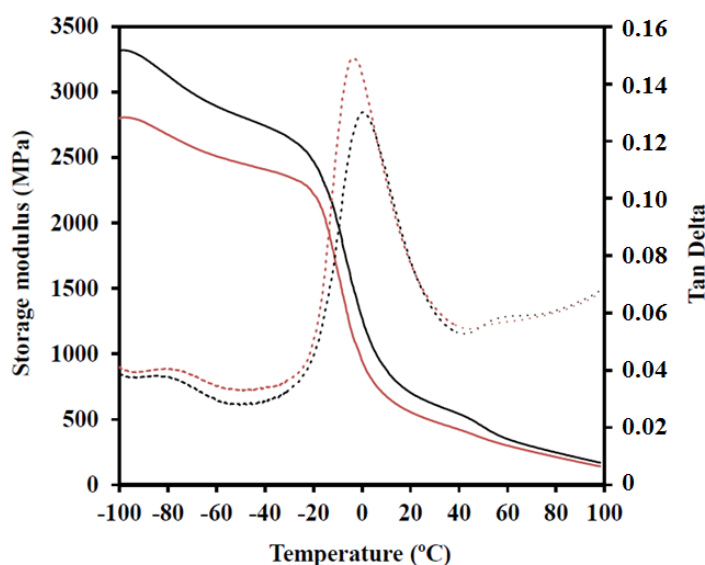
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505 **Figure 7.** Storage modulus (E') (solid line) and loss tangent (dashed line) curves of PBAAdT (red) and
 506 PBAAdT-HAp (blue) samples.

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Table 6. DMTA data of the studied copolyesters and nanocomposites.

Sample	T_g ($^\circ\text{C}$)	$E'_{-20^\circ\text{C}}$ (MPa)	$E'_{20^\circ\text{C}}$ (MPa)	E'_{70} (MPa)
PBSTS	10.5	1830	480	180
PBAAdT	-2.5	1840	550	250
PBSeT	-6.5	2030	370	80
PBST-HAp	11.0	2210	590	220
PBAAdT-HAp	2.3	2470	700	290
PBSeT-HAp	-3.5	2200	400	100

508 ^aStorage moduli are given for temperatures below ($-20\ ^\circ\text{C}$) and higher than ($20\ ^\circ\text{C}$) the first glass
 509 transition temperature and after the second glass transition temperature ($70\ ^\circ\text{C}$).

510 3.5. Contact angle measurements

511 Contact angles of water droplets on films of the three copolymers were similar (i.e. between 83°
 512 and 85° as shown in Figure 8). Therefore, the change of the aliphatic dicarboxylic unit (i.e. the

number of methylene groups) did not greatly affect the final hydrophobicity. In general, these surfaces could be considered in the borderline (90°) between hydrophobic and hydrophilic characters. It should be pointed out that the ratio of these aliphatic units was low (30% of the total dicarboxylic content) and probably a minimum influence of composition should be expected. On the contrary, a significant decrease up to 72°-78° (Figure 8) was observed when HAp was incorporated. In this case, some differences were found for the three derivatives, as the hydrophobicity slightly increased with increase in the methylene content. The result is meaningful since degradability can be enhanced as a consequence of a higher hydrophilicity.

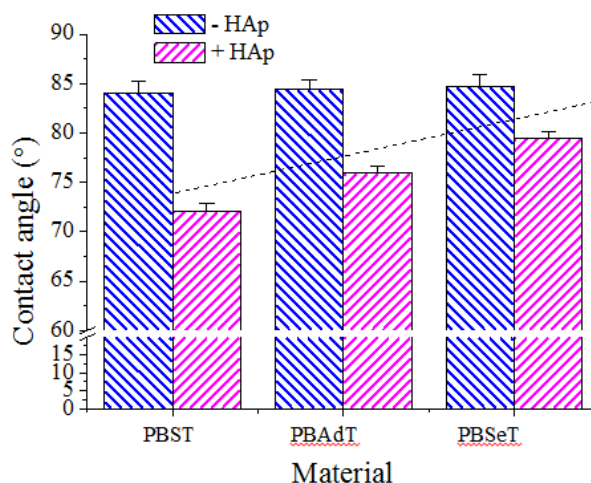


Figure 8. Contact angle measurements for water on films of PBST-HAp, PBAdT-HAp, PBSeT-HAp nanocomposites and the corresponding HAp free samples.

3.6. Cell adhesion and proliferation

Figure 9 shows the adhesion and proliferation results corresponding to different samples, making use of both epithelial-like and fibroblast-like cell lines (MDCK and COS-7 cells, respectively). A similar cell adhesion of fibroblasts (close to 80%) was found for the three studied copolyesters but interestingly it was slightly increased up to 90%-95% when HAp was incorporated. The results are significant since demonstrated that biocompatible characteristics of PBT can be improved by the addition of HAp and that aliphatic dicarboxylic units may play an important role in such observation. Note that the highest viability was detected for derivatives with longer adipic (90%) and sebacic acid (95%) units (Figure 9a). These results may be a consequence of the increased hydrophobicity of samples with longer aliphatic units.

Effects on adhesion were more evident when epithelial-like cells were employed since succinate and adipate compounds were associated with a statistically lower value (< 80%) compared to the control, while the adhesion increased in the range of 80-95% for the sebacic acid derivative and also for all HAp composites (Figure 9c).

Experimental results could be explained by the fact that epithelial cells form a monolayer of flat cells with a polygonal/irregular shape and hence are in close contact, giving rise to apical and basolateral domains. In fact, the monolayer can be considered as a barrier between the material surface and the culture medium. Epithelial cells need a suitable material surface to adhere through the basal domain and consequently are highly sensitive to inappropriate surfaces. On the contrary, fibroblast cells are characterized with their high mobility (i.e. they can easily contract and extend) since do not form such monolayer. Furthermore, there is no limitation in interchange between the material surface and the medium due to the absence of apical and basolateral domains. Probably, polymers having short dicarboxylic units may cause an acidification of the culture medium and a reduction of viability. The incorporation of HAp may damp this acidification since calcium phosphate can be considered as a buffering agent. On the other hand, it is well-known that cellular

560 adhesion is improved when Ca^{2+} and Mg^{2+} cations are present, the former one being provided by
 561 HAp particles.
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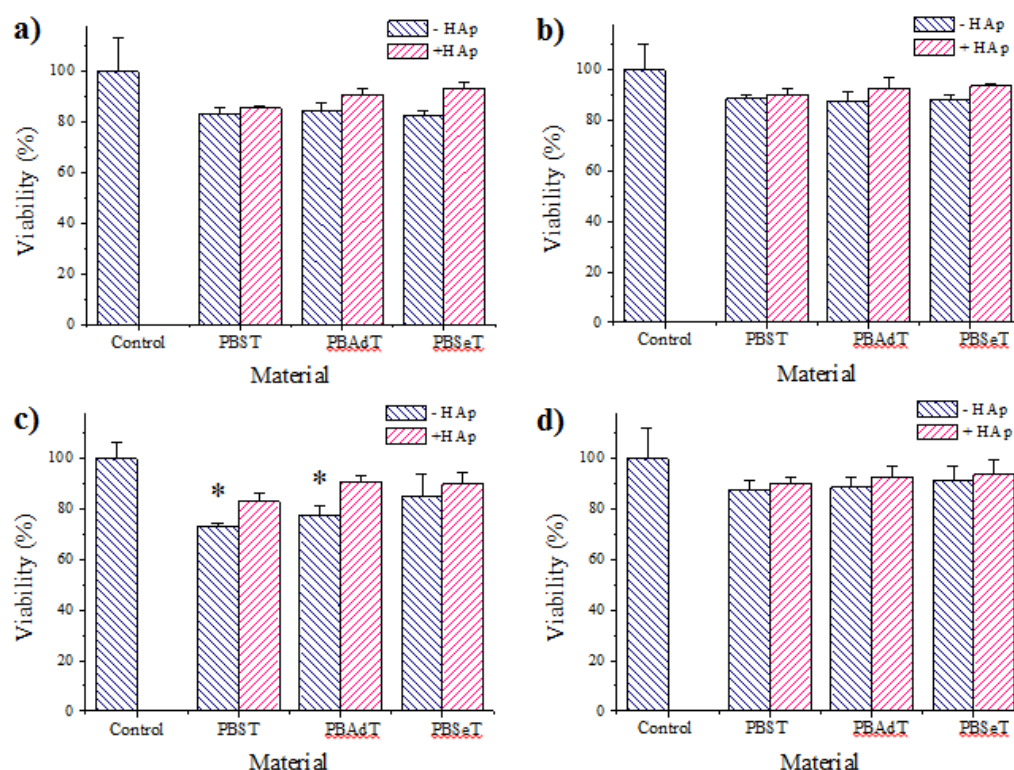
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583 **Figure 9.** Adhesion (a,c) and proliferation (b,d) onto materials of: a-b) COS-7 (fibroblast-like cells),
 584 c-d) MDCK (epithelial-like cells). Asterisks $p < 0.05$ using Tukey-test.

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Proliferation results were similar for both fibroblast and epithelial cell lines (Figures 9b and 9d, respectively), a feature probably indicated that cell morphology is not crucial for long time (7 days) events. In general, results were satisfactory for all samples (viability in the 85-95% range), although a slight improvement was observed again when HAp was incorporated.

These results are qualitatively shown in Figure 10. The epithelial cells form monolayers were organized into cellular clusters on the surface of the three copolymers (Figures 10a-10c). Fibroblasts are more segregated on the surface of the copolymers and their cytoplasm extends with fusiform shapes (see arrows in Figures 10d-10f). These characteristics of cell-surface interactions are typical for each cell type when cytoskeleton is reorganized. Figures 10g-10k show epithelial cells from an early interaction (as evidenced by its spherical shape) with the copolymer surface so as to form lamellipodia by extending their cytoplasm. Cells tended toward a flat shape and their base was fully extended on the copolymer surface (Figure 10i). This widespread adherence to the surface was achieved by multiple tiny hairs ($< 1 \mu\text{m}$) that emerged from the membrane (Figure 10k). In contrast, fibroblast cells attach to the copolymers surface in a more localized manner. Long cytoplasmic extensions allowed colonizing large area of the material surface while interacted with other cells (Figure 10l). However, it is clear that multiple filopodia of different lengths (clearly $> 1 \mu\text{m}$) emerged from the cytoplasmic extensions (Figures 10m-10n). These filopodia were multi-filaments that become separated when interacting with the material. The fingers-like structures (Figures 10o-10p) gave rise to a good adhesion by appropriate anchoring onto the material.

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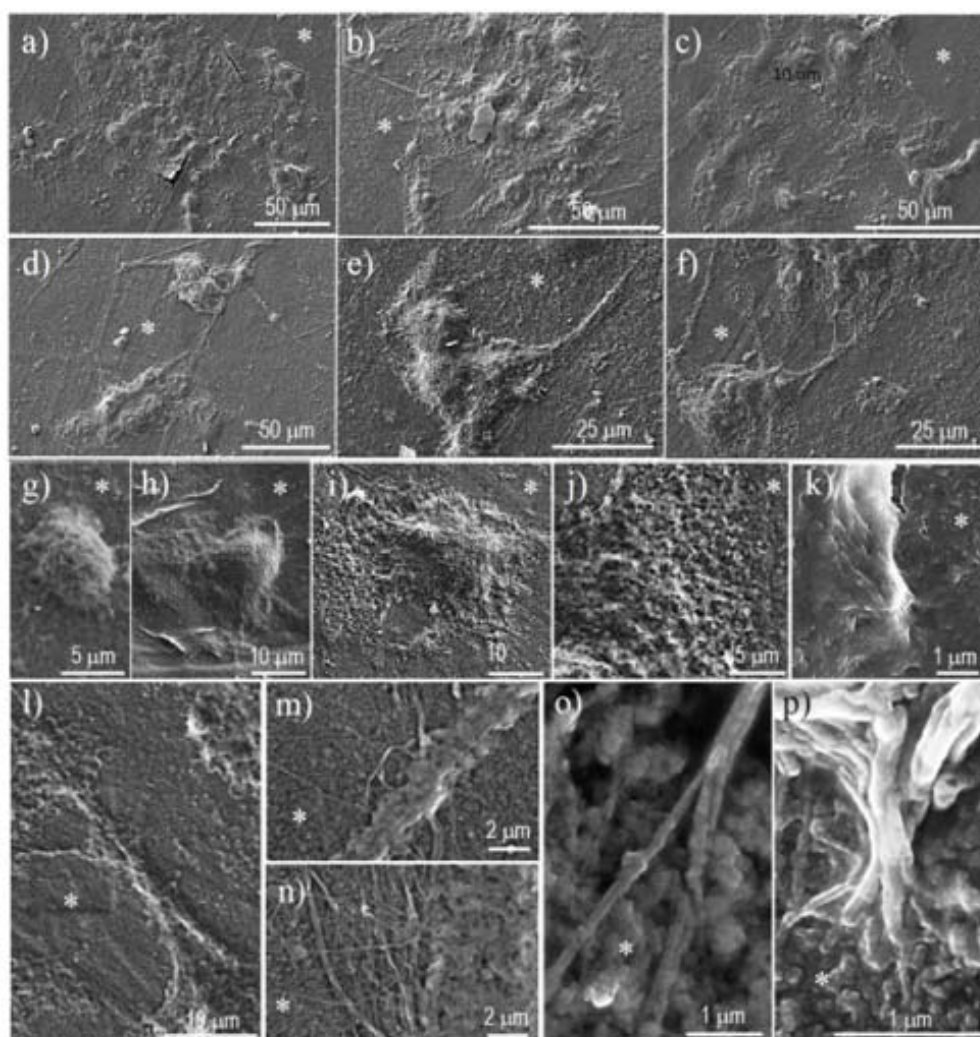
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621 **Figure 10.** Epithelial-like MDCK cells adhered on PBST-HAp (a), PBAAdT-HAp (b), and PBSeT-HAp
 622 (c). Fibroblast-like COS-7 cells adhered on PBST-HAp (d), PBAAdT-HAp (e), and PBSeT-HAp (f).
 623 Overall details of the cellular adhesion of epithelial-like cells (g-k) and fibroblast-like cells (l-p).
 624 Asterisk indicates the material surface. Arrows are described in the text.

625 3.7. Hydrolytic degradation

626 Figure 11 shows the evolution of the remaining weight percentage of the studied copolyester
 627 films during exposure to a pH 7.4 aqueous medium under accelerated conditions provided by a
 628 temperature of 70 °C. It is clear that all samples were hydrolytically degradable since the weight loss
 629 after 60 days of exposure ranged between 31% and 48%. Degradation obviously proceeded at a
 630 slower rate when temperature was decreased to 37 °C. In this case, weight loss values were lower
 631 than 5% (data not shown). The three copolyesters were different in terms of their degradation. In
 632 aliphatic-aromatic copolyesters, the melting behaviour is mainly determined by the length of
 633 aromatic sequences in the polymer chains, which depends both on the composition and the
 634 structure. Besides the fixation of the polymer chains in the crystalline domains, the flexibility of the
 635 chain itself also influences the degradation behaviour to some extent. Hydrolytic and enzymatic
 636 degradation of poly(butylene succinate) and its copolymers have recently been reviewed, being
 637 emphasized the great influence of the low flexibility of polymer chains on their relatively slow

638 hydrolysis rate [31]. Therefore, copolyesters with long aliphatic dicarboxylic acids exhibit a
 639 somewhat higher degradation rate than those with shorter ones [10], however, this effect usually is
 640 masked by the much higher influence of the melting point. Degradation products of poly (butylene
 641 succinate-co-terephthalate) after enzymatic hydrolysis has been analysed and the water-soluble
 642 oligomers up to hexamer were detected after the hydrolysis. The oligomeric fragments were slowly
 643 hydrolysed by secondary hydrolysis into 4-hydroxyl succinate and terephthalate [32]. Therefore
 644 contrary to the expectations about the length of the dicarboxylic content, the lowest weight loss for
 645 the sebacate derivative could be attributed to more insolubility of the degradation fragments.

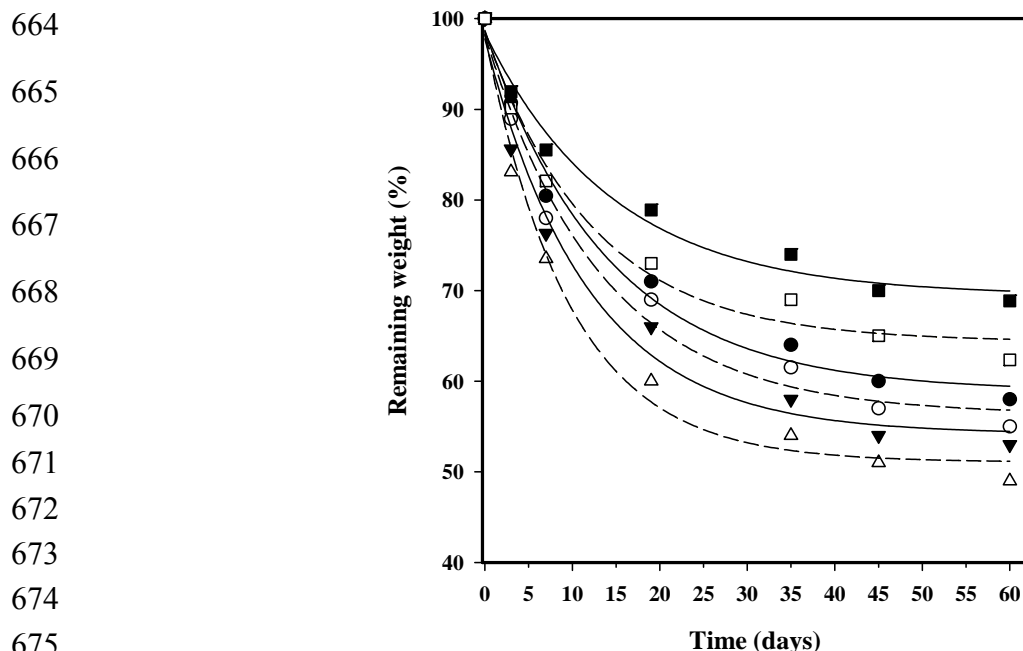
646 Incorporation of HAp caused an increase in degradability compared to the parent copolyester,
 647 which could be explained by the increase in hydrophilicity. After 60 days of exposure, the weight
 648 loss increased by 4%-7% with respect to the parent copolyester, where the higher percentage was
 649 related to the less degradable PBSeT-HAp sample. It seems that the effect caused by the hydrophilic
 650 HAp particles was more relevant when the polymer matrix was more hydrophobic.

651 Average molecular weight during exposure to the 70 °C medium is shown in Figure 12a for
 652 PBAdT and PBAdT-HAp samples. In this case, the degradation process is more evident than that
 653 observed from weight loss measurements. In fact, molecular weight rapidly decreased, reaching a
 654 practically constant M_n value of 1200-750 g/mol after only 19 days of exposure. In this case, the
 655 differences between copolyesters and their nanocomposites were scarce (data not shown), due to the
 656 rapid change in the molecular weight.

657 A first order degradation mechanism was assumed to quantify and compare the degradation
 658 rate of different samples. In fact, hydrolytic degradation of polyesters in the early stages has been
 659 usually simulated based on a exposure time dependence of molecular weight given by equation
 660 5:^{33,34}

$$661 \quad M = M_0 e^{-kt} \quad (7)$$

662 where M is the molecular weight at time t , M_0 is the initial molecular weight and k indicates the
 663 kinetic constant.



676 **Figure 11.** Plot of the variation of the remaining weight percentage during exposure time to a pH 7.4
 677 hydrolytic medium at 70 °C for succinic (circles), adipic (triangles) and sebacic (squares) acid
 678 copolyesters with (open symbols) and without (full symbols) HAp.

679 Figure 12a shows a good fit between experimental and simulated data for both number and
 680 weight average molecular weights when the exposure time was low, and a clear deviation at times
 681 longer than 7 days. It is clear that molecular weight tended to asymptotic values, which should be
 682 related to the molecular size required to get soluble fragments. Obviously, the kinetic approximation
 683 was not correct for high exposure times.

684 Values of kinetic constants clearly showed an increase when HAp was incorporated.
 685 Specifically, the values determined for PBAdT increased from 0.039 days⁻¹ to 0.048 days⁻¹ when the
 686 number average molecular weights were considered, and from 0.045 days⁻¹ to 0.055 days⁻¹ when M_w
 687 data were used.

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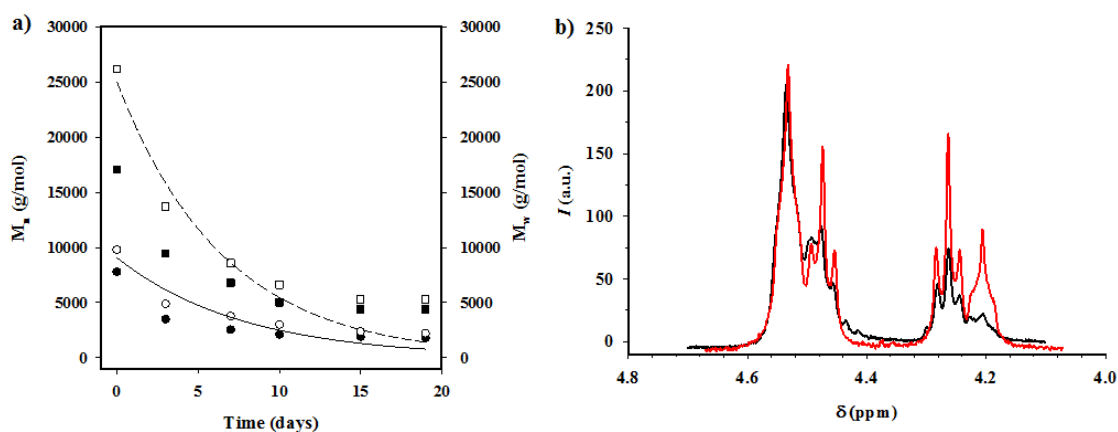
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701 **Figure 12.** a) Plot of the variation of the number (solid line) and weight (dashed line) average
 702 molecular weight of PBAdT and PBAdT-HAp samples during exposure time to the hydrolytic
 703 medium at 70 °C as simulated considering a first order degradation mechanism. Experimental data
 704 (squares and circles for M_w and M_n , respectively) taken during degradation are shown for both the
 705 copolyester (full symbols) and the nanocomposite (open symbols). b) ¹H NMR spectrum of a PBAdT
 706 samples before (red line) and after exposure (black line) for 60 days to the hydrolytic medium at 70
 707 °C.

708 Analysis of the NMR spectra of degraded samples (Figure 12b) showed a great decrease in the
 709 peak associated with the ABA sequence, demonstrating that degradation mainly occurred through
 710 the aliphatic units as might be presumed.

711 SEM micrographs revealed that hydrolytic degradation mainly took place in the inner parts of
 712 the exposed films due to a local concentration of acidic degradation products. Figure 13 shows the
 713 initial film surface of the PBAdT representative sample and details of films after exposure for 60
 714 days to the hydrolytic medium. It is clear that the initial smooth surface (Figure 13a) evolves into the
 715 formation of cracks (Figure 13b) with interconnecting fibers (Figure 13d) and sinking of the surface
 716 (Figure 13c, 13e and 13f). This is caused by the development of deep inner holes (Figure 13g) that end
 717 up affecting the surface appearance (Figure 13h).

718 3.8. Enzymatic degradation

719 Enzymatic degradation studies indicated that the three copolymers were susceptible to lipases
 720 attack (Figure 14). The degradation rate was slow but steadily progressed with exposure time. In
 721 general, the weight loss was between 16.5% and 15.5% after 55 days of exposure to *Pseudomonas*
 722 *cepacia*, the values being slightly lower for the porcine lipase medium (i.e. from 15.5% to 11%). In any
 723 case, trends were similar and specifically the highest and lowest weight losses were found for the
 724 adipic and the sebacic acid derivatives, respectively. Results are in agreement with those attained for
 725 hydrolytic degradation and probably are not a consequence of a specificity of selected enzymes
 726 towards the polymer substrate. Interestingly, the incorporation of HAp nanoparticles increased the
 727 enzymatic degradability of all samples, being the effect more pronounced for the adipic derivative.
 728 Thus in this case, weight loss increased from 16.5% to 20% after 55 days of exposure.

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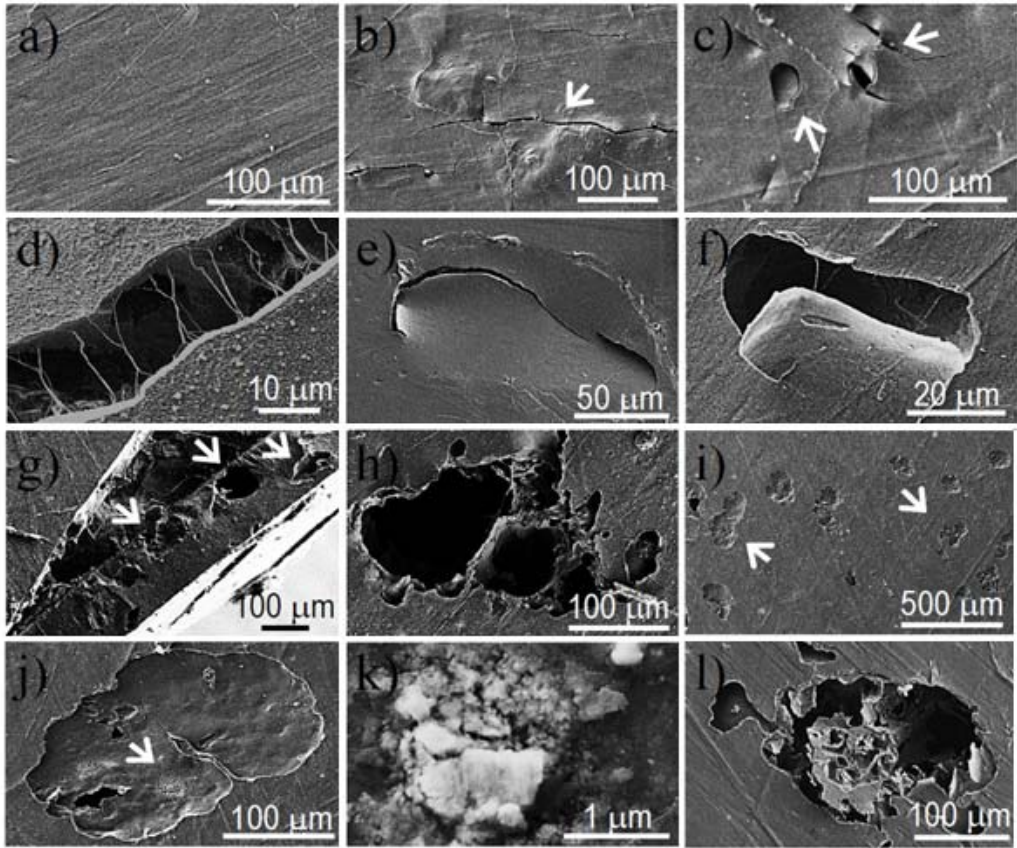


Figure 13. SEM micrographs showing the surface of PBAdT films at the beginning and after exposure to a pH 7.4 aqueous medium at 70 °C for 60 days (b-h) and to a *Pseudomonas cepacia* enzymatic medium for 52 days (i-l).

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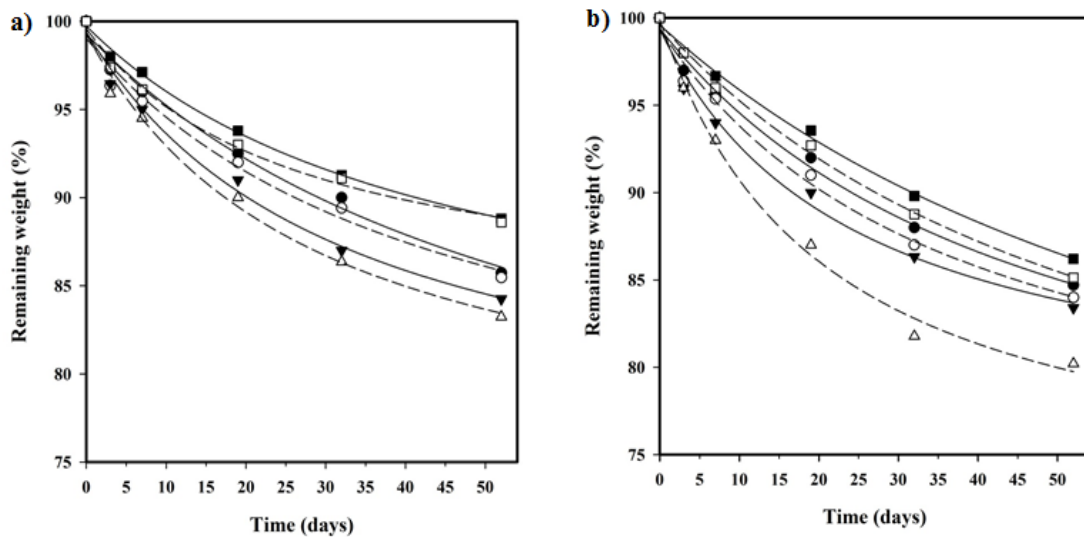


Figure 14. Plot of the variation in the remaining weight percentage during exposure time to enzymatic media of lipases from porcine (a) and *Pseudomonas cepacia* (b) for succinic (circles), adipic (triangles) and sebacic acid (squares) copolyesters with (open symbols) and without (full symbols) HAp.

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The progress of degradation was also examined using SEM and the micrographs corresponding to large exposure times (Figures 13i-13l) showed different degrees of surface erosion. This could lead

773 to concavities (Figures 13i and 13j) where in some cases, degradation products could be retained
774 (Figure 13k), and deep holes could justify the observed weight losses (Figure 13l). These eroded
775 surfaces contrast with the smooth appearance of the initial films (Figure 13a).

776 Contact angle measurements on the surface of exposed films revealed a significant increase in
777 the hydrophilicity, consistent with the degradation process. For instance, 30°, 44°, 64° angles (not
778 shown) were determined for PBA_dT-HAp, PBST-HAp and PBSeT-HAp samples after exposure for
779 55 days, respectively. In this way, the surface of films was enriched with hydrophilic terminal
780 groups generated by the degradation process. Furthermore, reduction in the contact angle from the
781 values previously determined for non-exposed samples (i.e. 78.3°-72° as shown in Figure 8) suggest
782 that adipic and sebacic acid derivatives were the most and less degraded samples, respectively.

783 4. Conclusions

784 Poly (butylene terephthalate-*co*-aliphatic dicarboxylate)s having succinate, adipate or sebacate
785 acid units as aliphatic moieties could be obtained with a random distribution from the
786 corresponding aromatic and aliphatic prepolymers (i.e. PBT and PBA). Transesterification reactions
787 took place at 250 °C in a sufficient extension to render a random microstructure as detected by NMR
788 sequence analyses.

789 Incorporation of HAp nanoparticles in the reaction medium gave rise to grafting reactions
790 between the hydroxyl groups placed on the HAp surface and the carboxyl terminal groups of
791 polymer chains. A considerable fraction of polymer became insoluble due to the crosslinking process
792 whereas the soluble fraction revealed a significant increase of molecular weight as a consequence of
793 the grafting reactions.

794 HAp had a clear influence on the thermal stability and specifically caused a stabilization that
795 could reflect the decrease in terminal carboxylic groups as a consequence of the grafting reactions.

796 Incorporation of nanoparticles increased the elastic modulus of the samples and more
797 interestingly their biocompatibility. HAp also increased the hydrophilicity of the sample surface,
798 which is a crucial factor that allowed enhancing both enzymatic and hydrolytic degradability.
799 Degradation rate slightly varied depending on the aliphatic dicarboxylic unit. Specifically, adipic
800 and sebacic acid derivatives gave rise to the highest and lowest rates in all assayed media,
801 respectively.

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805 Author Contributions

806 All authors made contributions to the development of this manuscript and approved the final
807 manuscript. Nina Heidarzadeh contributed to the experimental work and the initial draft, Faramarz
808 A. Taromi to the polymer synthesis, Lourdes Franco to calorimetric analyses, Luís J. del Valle
809 assisted with degradation and biological experiments and both, Mehdi Rafizadeh and Jordi Puiggali
810 contributed to the concept, analyses of data and design and revision of the manuscript.

811 Conflicts of Interest

812 The authors declare no conflict of interest.

813 References

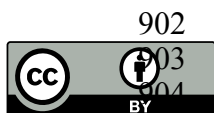
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