

**Physiologically-based pharmacokinetic
modelling and simulation of oral drug
bioavailability: Focus on bariatric
surgery patients and mechanism-based
inhibition of gut wall metabolism**

**A thesis submitted to the University of Manchester for the
degree of Doctor of Philosophy in the Faculty of Medical
and Human Sciences**

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Abstract

THE UNIVERSITY OF MANCHESTER,

Abstract of thesis submitted by Adam S. Darwich, for the degree of PhD and entitled:
"Physiologically-based pharmacokinetic modelling and simulation of oral drug bioavailability: Focus on bariatric surgery patients and mechanism-based inhibition of gut wall metabolism"

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Understanding the processes that govern pre-systemic drug absorption and elimination is of high importance in pharmaceutical research and development, and clinical pharmacotherapy, as the oral route remains the most frequently used route of drug administration. The emergence of systems pharmacology has enabled the utilisation of *in silico* physiologically-based pharmacokinetic (PBPK) modelling and simulation (M&S) coupled to *in vitro-in vivo* extrapolation in order to perform extrapolation and exploratory M&S in special populations and scenarios where concerns regarding alterations in oral drug exposure may arise, such as following gastrointestinal (GI) surgery or metabolic drug-drug interactions (DDIs).

Due to the multi-factorial physiological implications of bariatric surgery, resulting in the partial resection of the GI tract, the inability to rationalise and predict trends in oral drug bioavailability (F_{oral}) following surgery present considerable pharmacotherapeutic challenges. PBPK M&S is a highly implemented approach for the prediction of DDIs. Reoccurring issues have emerged with regards to predictions of the magnitude of mechanism-based inhibition (MBI) where overestimations of DDIs have repeatedly been reported for drugs exhibiting high intestinal extraction.

The aim of this thesis was to explore the interplay between oral drug absorption and metabolism occurring in the GI tract through the exploration of the impact of bariatric surgery on oral drug exposure and by theoretically examining the nesting and hierarchy of enterocyte and enzyme turnover and its impact on MBIs in the small intestine. This would be carried out by utilising a systems pharmacology PBPK M&S approach under a general model development framework of identification and characterisation of critical intrinsic factors and parameters, model implementation and validation.

Developed post bariatric surgery PBPK models allow a framework to theoretically explore physiological mechanisms associated with altered oral drug exposure pre to post surgery, which could be assigned to the interplay between dissolution, absorption and gut-wall metabolism, where dissolution and formulation properties emerged as the perhaps most important parameters in predicting the drug disposition following surgery. Model validation identified missing critical factors that are essential for additional model refinement. Developed post bariatric surgery PBPK models have the potential of aiding clinical pharmacotherapy and decision-making following surgery. A mechanistic PBPK model was developed to describe the hierarchical dependency of enzyme and enterocyte turnover in the small intestine. Predicted enzyme recovery using the nested enzyme-within-enterocyte turnover model may potentially account for reported overpredictions of mechanism-based inhibition. Developed models in this thesis showcase the advantage of PBPK M&S in the extrapolation of oral drug exposure to special population and the potential of a PBPK approach in understanding underlying the underlying mechanism governing F_{oral} and additionally highlight the need for generation of interdisciplinary data to support model development.

Declaration

No portion of the work referred to in this thesis has been submitted in support of an application for another degree or qualification of this or any other university or other institute of learning.

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List of abbreviations

A: Surface area

A_{CYP}: Abundance of Cytochrome P450

A_{diss}: Amount dissolved drug

A_{Ent-n/0}: Ratio of enzyme activity using the NEWE model compared to the conventional modelling approach

A_{Enz}: Amount of active enzyme

A_n: Amount of drug

A_{undis}: Amount undissolved drug

ACAT: Advanced compartmental absorption and transit

ACE: Angiotensin-converting-enzyme

ADAM: Advanced dissolution absorption and metabolism

ADME: Absorption, distribution, metabolism and elimination

AGBD: Adjustable gastric band

AGP: α -1 Acid Glycoprotein

AIDS: Acquired immunodeficiency syndrome

AUC: Area-under-curve

BCRP: Breast cancer resistance protein

BCS: Biopharmaceutics classification system

BDDCS: Biopharmaceutics drug disposition classification system

BMI: Body mass index

BPD: Biliopancreatic diversion

BPD-DS: Biliopancreatic diversion with duodenal switch

BSA: Body surface area

C: Concentration

C_{ent}: Enterocyte concentration

Caco-2: Colorectal adenocarcinoma-2 cells

CAT: Compartmental absorption and transit

CI: Confidence interval

CLogP: Calculated logP

C_{max}: Maximum concentration

C_{mic}: Concentration of microsomal protein in the assay

C_s : Solubility over the physiological pH range
 CL: Clearance
 CL_{int} : Intrinsic clearance
 $CL_{u_{int}}$: Intrinsic unbound clearance
 CL_{PD} : Passive diffusion clearance
 CNS: Central nervous system
 CR: Controlled release
 CV: Coefficient of variation
 CYP: Cytochrome P450

 D: Diffusion coefficient
 Do: Dose number
 DDI: Drug-drug interaction
 DR: Dissolution rate

 EC: Enteric-coated
 ER: Extended release

 f_a : Fraction of the absorbed dose that escapes gut wall metabolism
 F_G : Fraction of the absorbed dose that escapes gut wall metabolism
 F_H : fraction of the dose reaching the portal vein that escapes hepatic metabolism
 F_{oral} : Oral drug bioavailability
 FaSSIF: Fasted state simulated intestinal fluids
 FeSSIF: Fed state simulated intestinal fluids
 FDA: Food and drug administration
 f_u : Fraction of unbound substrate
 f_{u_b} : Fraction of unbound substrate in blood
 $f_{u_{Gut}}$: Fraction of unbound substrate in the gut
 $f_{u_{mic}}$: Fraction of unbound substrate in microsomes
 f_{u_p} : Fraction of unbound substrate in plasma

 GI: Gastrointestinal
 GFR: Glomerular filtration rate
 GM: Geometric mean
 GSD: Geometric standard deviation

GST: Glutathione S-transferases

h: Diffusion layer thickness

HA: Hepatic artery

HBA: Hydrogen-bond acceptors

HBD: Hydrogen-bond donors

HIV: Human immunodeficiency virus

HLM: Human liver microsomes

HSA: Human serum albumin

I: Inhibitor

IR: Immediate release

ISEF: Inter system expression factor

iv: Intravenous

IVIVC: *In vitro-in vivo* correlation

IVIVE: *In vitro-in vivo* extrapolation

J_{\max} : Maximum flux

JIB: Jejunoileal bypass

k_a : Rate of absorption

k_{deg} : Rate of turnover

$k_{\text{deg,CYP3A}}$: Rate of CYP3A4 turnover

$k_{\text{deg,Ent}}$: Rate of enterocyte turnover

$k_{\text{deg,Enz}}$: Rate of enzyme turnover

$K_{I,u}$: Unbound dissociation constant

$K_{i,u}$: Unbound inhibition constant

k_{inact} : Maximum rate of enzyme inactivation

K_m : The concentration at which half of the maximum velocity is reached

K_{reabs} : Reabsorption rate

k_{sit} : Small intestinal transit

k_{st} : Gastric emptying rate

k_t : Transit rate

K_p : Tissue to plasma partition coefficient

K_{pu} : Unbound tissue to plasma partition coefficient

L: Length
 LAGBD: Laparoscopic adjustable gastric band
 LLC-PK₁: Lilly Laboratory Cells – Porcine Kidney Nr. 1
 LogD: Logarithm of the distribution coefficient
 LogP: Logarithm of the partitioning coefficient

 M&S: Modelling and simulation
 M₀: Highest dose level of a given drug
 MBI: Mechanism-based inhibition
 MDCK: Madin-Darby canine kidney cells
 MDRD: Modification of diet in renal disease
 MPPI: Microsomal protein per intestine
 MPPGL: Microsomal protein per gram liver
 MRC: Medical Research Council
 MRP: Multidrug resistance-associated protein
 MW: Molecular weight

 NEWE: Nested enzyme-within-enterocyte
 NHS: National Health Services
 NSAID: Non-steroidal anti-inflammatory drug

 OATP: Organic anion transporting polypeptide

 ρ: Particle density
 P-gp: P-glycoprotein
 P_{app}: Apparent permeability
 P_{eff}: Effective permeability
 PAMPA: Parallel artificial membrane assay
 PBPK: Physiologically-based pharmacokinetics
 PEPT: Peptide transporter
 PhysChem: Physicochemical
 PK: Pharmacokinetics
 po: per oral
 PPI: Proton pump inhibitors
 ppR: Post/pre surgery oral drug exposure ratio

PSA: Polar surface area

Q: Flow

Q_{sec} : Secretory flow

QSAR: Quantitative structure-activity relationships

r: Radius

R_{syn} : Rate of synthesis

R&D: Research and development

REF: Relative expression factor

RYGB: Roux-en-Y gastric bypass

S: Substrate

S/C: Subcutaneous

S_{diss} : Solubility of drug in bile micelle media

SD: Standard deviation

SFM: Segregated flow model

SG: Sleeve gastrectomy

SIT: Small intestinal transit

SSRI: Selective serotonin reuptake inhibitor

SULT: Sulfotransferase

t: Time

$t_{1/2}$: Half-life

T_{lag} : Lag time

t_{max} : Time to reach maximum concentration

TCA: Tricyclic antidepressant

UGT: Uridine 5'-diphosphate-glucuronosyltransferase

V: Volume

V_{max} : Maximum velocity of reaction

V_o : Volume of co-administered fluid volume

V_{ss} : Volume of distribution at steady state following intravenous infusion

WHO: World Health Organisation

WX: Weighted combined geometric mean

Xd: Amount dissolved

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Chapter 1: Introduction

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Pharmacokinetics (PK) is defined as the processes that determine drug disposition in the body; these processes can conceptually be divided into absorption, distribution, metabolism and excretion (ADME) and will govern the exposure of a given drug at the site of measurement and effect (Rowland and Tozer, 1989).

The fundamental concept of the drug dose-effect relationship warrants the necessity to measure drug concentration *in vivo* over time in order to quantify this relation. Utilising mathematical models drug specific PK parameters can be estimated for a given population, an approach referred to as compartmental PK modelling. In pharmaceutical research and development (R&D) it is however desirable to be able to extrapolate and predict drug disposition throughout R&D in order to inform decision making, this includes the prediction of PK in pre-clinical species and man from *in vitro* data, referred to as *in vitro-in vivo* extrapolation (IVIVE), extrapolation of PK from pre-clinical species to man, and the prediction of PK in special disease populations from healthy volunteers (Rowland and Tozer, 1989; Rowland *et al.*, 2011; Rostami-Hodjegan, 2012).

Physiologically-based pharmacokinetic (PBPK) modelling and simulation (M&S) assign physiological meaning to compartmental models from population specific systems parameters as well as drug specific parameters, such as permeability and metabolism, that may be informed via IVIVE and *in vitro-in vivo* correlation (IVIVC). This approach of coupling IVIVE to PBPK modelling is often referred to as systems pharmacology (Rowland *et al.*, 2011; Rostami-Hodjegan, 2012).

Understanding the processes that determine pre-systemic drug absorption and elimination is a pivotal part of PBPK M&S and a constant focus of research as the oral route of drug administration remains the most frequently utilised due to its convenience and cost-efficiency (Bartholow, 2010; FDA, 2010).

The focus of the work in this thesis is on the PBPK M&S of the interplay between oral drug absorption and metabolism occurring in the gastrointestinal (GI) tract with a particular interest in special subpopulations, namely bariatric surgery patients and the theoretical

modelling of nested enzyme-within-enterocyte turnover, in order to improve the prediction of metabolic drug-drug interactions (DDIs) in the small intestine.

1.1 Oral drug bioavailability

Oral drug bioavailability (F_{oral}) is the product of three consecutive processes occurring following oral administration, the availability of the drug at each stage is defined as: The fraction of the administered dose that is absorbed into the gut wall (f_a), the fraction of the absorbed dose that escapes gut wall metabolism (F_G) and the fraction of the dose available to the portal vein that escapes hepatic metabolism (F_H) (Equation 1.1). The GI component ($f_a \cdot F_G$) of F_{oral} will be dependent upon a combination of systems, drug and formulation specific parameters.

$$F_{oral} = f_a \cdot F_G \cdot F_H$$

Equation 1.1: Components of F_{oral} .

Where F_{oral} can be determined experimentally in man as the ratio of the dose normalised area-under-curve (AUC) of a per oral (po) over that of the intravenous (iv) dose (Equation 1.2). The determination of human f_a and F_G will however typically rely on indirect methods of measure such as extrapolation from pre-clinical species to man, static or dynamic *in silico* modelling approaches (Rowland and Tozer, 1989; Yang *et al.*, 2007b).

$$F_{oral} = \frac{AUC_{po} \cdot Dose_{iv}}{AUC_{iv} \cdot Dose_{po}}$$

Equation 1.2: Experimental determination of F_{oral} .

1.1.1 Gastrointestinal systems parameters

The GI systems parameters that may influence F_{oral} comprise a number of intrinsic processes concerning the absorption of nutrients and the repulsion and metabolism of xenobiotics, including among others: Gastric emptying, intestinal motility and transit, luminal fluid dynamics, intestinal absorption area, abundances and regional distribution patterns of drug metabolising enzymes and transporters. Underneath follows an account of the most relevant factors and their impact on F_{oral} .

Gastric emptying and intestinal transit

Under normal conditions the gastric emptying half-life is approximately 0.24 hours following liquid intake with a coefficient of variation (CV) of 38%. A variety of factors may affect gastric emptying, including: the prandial state, composition and volume of the consumed meal or liquid, drugs (anticholinergics and opioid-analgesics amongst others), disease states and surgical procedures (diabetes, gastric ulceration, bariatric surgery and more) (Barowsky *et al.*, 1965; Horowitz *et al.*, 1982; Oberle *et al.*, 1990; Murphy *et al.*, 1997; Samsom *et al.*, 2003; Kamdem *et al.*, 2005; Hellmig *et al.*, 2006; Jamei *et al.*, 2009; Ogungbenro *et al.*, 2011). For highly permeable, highly soluble compounds gastric emptying becomes the rate-limiting step for absorption, thus potentially altering the time for the drug to reach the maximum systemic concentration (t_{\max}), the maximum concentration (C_{\max}) and f_a .

Small intestinal transit displays a mean of approximately 3.32 h, conforming to a logit-normal distribution pattern in the population (Yu *et al.*, 1996). A number of special disease subpopulations display altered small intestinal motility, including: Patients suffering from cystic fibrosis, AIDS, liver cirrhosis, portal hypertension and post bariatric surgery patients, amongst others (Sharpstone *et al.*, 1999; Karlsen *et al.*, 2012; Dirksen *et al.*, 2013). Small intestinal transit time may influence the absorption of solubility and permeability limited compounds or drugs given as extended-release formulation. Rapid transit through the small intestine may postpone the absorption process further distally and therefore limit the rate of absorption (k_a) and f_a (Rowland and Tozer, 1989).

The colonic transit time (~24 h) is considered to be of less significance for oral drug delivery as compared to the small intestine, where the colon displays a reduced capacity for absorption and dissolution. The colon is however a target for many controlled release formulations where the release may extend for up to 24 h (Hardy *et al.*, 1985; Schiller *et al.*, 2005; Tannergren *et al.*, 2009).

Gastrointestinal fluid volumes, composition and pH

GI fluid volumes, composition and pH are fundamental determinants for the amount of drug that will be dissolved, and consecutively absorbed, in the GI tract, especially for solubility limited compounds. Approximately seven litres of fluids are secreted daily from the GI tract in man in the form of saliva, gastric and pancreatic juices, bile and more (Valentin, 2002).

The amount of fluid available to dissolve a given drug will be determined by: Fluid intake, GI secretion, transit and reabsorption. Levels of measured fluid content under fasted condition amount to approximately 45 mL in the stomach with a standard deviation (SD) of 18 mL, 105 (± 72) mL and 13 (± 12) mL in the small intestine and colon respectively thus exhibiting considerable inter-individual variability (Schiller *et al.*, 2005; Sutton, 2009).

Bile micelle mediated solubilisation can act to greatly enhance the solubilisation and dissolution rate of highly lipophilic compounds. The extent at which bile mediated solubilisation occurs is related to concentration of bile salt in the small intestine, where bile is released at a rate of approximately 1.5-15.4 $\mu\text{L}/\text{min}/\text{kg}$ in man (Sugano, 2009). Following secretion into the duodenum, the bile will be subject to dilution in luminal contents and reabsorption throughout the intestine, this results in a gradient where the bile salt concentration is reducing further distally along the small intestine. In the fasted state the bile salt concentration will be approximately 2 to 6.2 mM. Upon post-prandial triggered release the bile concentration can vary between 0.5 and 37 mM in man. Biliary secretion may act as a clearance route, eliminating drug from the system via the liver into the duodenum, mediated by active transport from the canicular membrane of the liver into the bile caniculus. Several transporters can act to mediate biliary secretion of drugs, including: P-glycoprotein (P-gp), multidrug resistance protein 2 (MRP2) and breast cancer resistance protein (BCRP) and a number of transporters involved in the biliary excretion of endogenous compounds (Funk, 2008; Holm *et al.*, 2013).

The GI pH varies widely across the stomach and small intestine, where the gastric pH sits between 1.7 and 5.0 in fasted and fed state respectively. The release of pancreatic juices by the gall bladder into the duodenum triggers an increase in the small intestinal pH, where it displays an increase distally from a pH of approximately 5-7 in the duodenum to 7.5 in the terminal ileum, pH is reduced in the caecum (pH 5.5-7.5), then increases further distally along the colon and in rectum (pH 6.1-7.5) (Karakli, 1995; Nugent *et al.*, 2001). Acid secretion and pH may vary in special disease populations, such as those suffering inflammatory bowel disease or following gastric resection thus potentially affecting oral drug absorption in these groups (Behrns *et al.*, 1994; Nugent *et al.*, 2001). pH plays a vital role in regulating the dissolution of orally administered compounds. Oral absorption of permeability limited drugs displaying a pK_a within the range of the GI pH may be highly influenced by pH

fluctuations, where an acid compound may display an increase in solubility at a higher pH and an alkaline compound may display a reduced solubility as a result of an increase in pH (Rowland and Tozer, 1989).

The GI tract is populated by approximately 400-500 different bacterial species (Moore and Holdeman, 1975). The level of bacterial microflora is low in the stomach and proximal small intestine but increases considerably distally towards colon and rectum (Kararli, 1995).

Bacterial microflora may facilitate presystemic clearance of orally administered drugs, thus reducing f_a , or can metabolise pro-drugs to active compounds and hydrolyse glucuronide conjugates excreted via biliary secretion thus facilitating enterohepatic circulation via reabsorption of parent compounds (Goldman, 1978; Pollack *et al.*, 1994; Chourasia and Jain, 2004).

Gastrointestinal hormones

A growing body of evidence has emerged over the last decade highlighting the importance of endogenous hormones in regulating gastrointestinal motility and behaviour in the prandial states. Gastric hormones, such as motilin and xenin, are released during the fasted state stimulating gastric emptying and potentially inhibiting gastric acid secretion, pancreatic secretion and intestinal motility. Food intake will trigger a cascade of post-prandial hormonal release, including GI hormones such as: ghrelin, gastrin, cholecystokinin, peptide YY and more, altering gastric emptying, acid secretion, intestinal fluid secretion and motility (Sanger and Lee, 2008). GI hormone responses have been reported to vary in special subpopulations, such as following bariatric surgery where the potential implications of these alterations may be crucial for determining oral nutrient and drug absorption in these populations (Savage *et al.*, 1987; Beckman *et al.*, 2011).

Absorption area

The absorption area of the small intestine directly affects f_a of orally administered drugs. The folding and villi structure of the small intestine helps to optimise the number of enterocytes that are exposed to the gut lumen and therefore can facilitate absorption. Several conditions do however reduce the absorption potential of oral nutrients and drugs due to a reduction in the length of the small intestine. These include: Short bowel syndrome and bariatric surgery.

Disease states can further alter the morphology of the villi, thus reducing the absorption area of the small intestine, such as the case for coeliac disease where a flattening of the villi structure is observed. A reduced absorption area may result in a reduced f_a of permeability limited drugs or delayed-release formulations (Parsons *et al.*, 1975; McFadden *et al.*, 1993; Bullen *et al.*, 2006; Padwal *et al.*, 2009).

Gut-wall metabolism

Small intestinal metabolism acts as a natural barrier for regulating F_{oral} of xenobiotics, despite the lower abundance of drug metabolising enzymes in the gut wall as compared to the liver, intestinal metabolism displays a metabolic capacity similar to the liver as a first line of exposure to orally administered drugs (Kolars *et al.*, 1994). Approximately 30% of orally administered drugs on the market display an F_G below 0.8, thus highlighting the relevance of appropriate models for describing gut wall metabolism (Varma *et al.*, 2010).

Similarly to the liver, Cytochrome P450 (CYP) 3A4 is the predominant drug metabolising enzyme in the small intestine, accounting for approximately 80% of the small intestinal CYP abundance, preceding CYP2C9, CYP2C19, CYP2J2, CYP2D6 and CYP3A5 (Peters *et al.*, 1989; Paine *et al.*, 1997; Fisher *et al.*, 2001; Paine *et al.*, 2006; Riches *et al.*, 2009). The regional abundance of CYP3A varies along the small intestine, where it is expressed at lower levels in the duodenum, increasing in the jejunum to then reduce further distally towards the ileum (Paine *et al.*, 1997). Inter-individual variation in abundance and polymorphism of enzyme expression (such as that for CYP2C9, 2D6 and 3A5) provide considerable variability in gut-wall metabolism and F_G of high affinity substrates (Ingelman-Sundberg, 2005; Sconce *et al.*, 2005; Barter *et al.*, 2010). In addition to the CYPs, the intestine is also abundant in sulfotransferases (SULTs) and uridine 5'-diphosphate-glucuronosyltransferases (UGTs) drug metabolising isoforms, some of which are exclusive for the small intestine (Radominska-Pandya *et al.*, 1998; Riches *et al.*, 2009).

Active transport

Numerous transporters are present in the gut facilitating both active uptake and efflux at the apical and basolateral side of the enterocytes. P-gp is the perhaps most extensively studied transporter. In the intestine, P-gp facilitates active efflux from the enterocyte into the gut

lumen of substrate drugs, displaying a relative expression distribution pattern increasing from the proximal to the distal small intestine (Mouly and Paine, 2003). Other active transporters present in the small intestine include (amongst others): efflux transporters (*e.g.* MRP2 and BCRP), apical uptake transporters (*e.g.* organic anion transporting polypeptide 1A2 (OATP1A2) and peptide transporter 1 (PEPT1)), and basolateral transporters (*e.g.* Organic cation transporter 1 (OCT1) and MRP3) (Fromm *et al.*, 2000; Maliepaard *et al.*, 2001; Ziegler *et al.*, 2002; Englund *et al.*, 2006; Glaeser *et al.*, 2007). Inter-individual variability in transporter expression can contribute to observed variability in F_{oral} of substrate drugs and have been proposed to affect F_G via interaction with drug metabolising enzymes. Utilising a PBPK M&S approach, Darwich and co-workers, assessed the impact of CYP3A4 and P-gp interplay on F_G where a reduction in F_G was observed as a consequence of active efflux resulting in enzyme de-saturation, this was however limited to a parameter space where the substrate in question displayed a high affinity to both CYP3A3 and P-gp (Benet and Cummins, 2001; Darwich *et al.*, 2010; Giacomini *et al.*, 2010).

1.2 IVIVE and IVIVC of drug specific parameters

Numerous drug specific parameters are known to influence f_a and F_G following oral dose administration. Over the last decades, pharmaceutical R&D has moved towards more mechanistic models for predicting F_{oral} based on compound characteristics, with advances originating from across pharmaceutical disciplines.

At the most fundamental level, solubility and permeability are the two key drug specific parameters contributing to f_a . Solubility and permeability are both related to the chemical structure and physicochemical (PhysChem) properties of a given compound. As a consequence of the emergence of combinatorial chemistry and high-throughput screening for lead compounds in pharmaceutical R&D, the need to quantify the relation between molecular descriptors and oral drug dissolution and absorption resulted in the definition of ‘Lipinski’s rule of five’. Lipinski, and co-workers, identified a number of PhysChem parameter criteria associated with a favourable F_{oral} , these include: molecular weight ($\text{MW} < 500 \text{ g/mol}$), calculated octanol/water partitioning coefficient ($\text{CLogP} < 5$), number of hydrogen-bond donors ($\text{HBD} < 5$) and acceptors ($\text{HBA} < 10$). The ‘Lipinski’s rule of five’ has been highly utilised in pharmaceutical R&D to screen for compounds with advantageous oral PK (Lipinski *et al.*, 2001).

Amidon, and co-workers (1995), developed the biopharmaceutics classification system (BCS) for assessing F_{oral} for immediate-release formulation drugs based on their solubility and permeability characteristics. According to the BCS, the *in vivo* solubility criterion is defined as a dimensionless dose number (Do) equal to the highest dose level of a given drug (M_o) in 250 mL of aqueous buffer (V_o), all divided by the drug solubility over a physiological pH range (C_s ; Equation 1.3). According to the solubility criterion a drug is classed as solubility limited if $Do \geq 1$ (i.e. if the dose amount one attempts to theoretically dissolve in 250 mL buffer is greater than that allowed by the solubility over a physiological pH range) (Amidon *et al.*, 1995; FDA, 2000).

$$Do = \frac{M_o/V_o}{C_s}$$

Equation 1.3: Biopharmaceutics classification system: Dose number (Do) criterion.

A compound is defined as highly permeable if it has $f_a \geq 90\%$ in man or in pre-clinical species or via indirect measurement of f_a using *in vitro* assays. Combined with the solubility criterion this results in four classes of compounds (Amidon *et al.*, 1995; FDA, 2000):

- BCS class I: High solubility, high permeability,
- BCS class II: Low solubility, high permeability,
- BCS class III: High solubility, low permeability
- BCS class IV: Low solubility, low permeability.

The BCS provides a rationale for the relation between solubility, permeability and f_a and potentially any additional parameters that may influence F_{oral} . A BCS class I drug may be subject to variability in absorption due to gastric emptying as this will be the rate limiting step for its dissolution and absorption. For a BCS class II drug the dissolution rate is highly relevant in determining F_{oral} , thus making the GI constituents, surfactants, GI pH fluctuations and processes that may alter compound solubility important for determining *in vivo* absorption. Further, class II compounds are the most likely to display efflux transporter effects due to their low solubility (which prevents saturation of transporters in the intestine). The effect of high-fat meals may be of importance in determining F_{oral} of class II drugs in the

case where micelle formation may enhance solubility, e.g. cyclosporine (Yu *et al.*, 2002; Wu and Benet, 2005).

In the case of a BCS class III drug, permeability is the rate limiting step in determining F_{oral} , which will be highly dependent upon GI transit, fluid dynamics and constituents, and the effective permeability. Class III compounds are the most likely to be sensitive to active uptake transporters in the GI tract due to the high level of drug available for uptake following dissolution in the small intestine (Yu *et al.*, 2002; Wu and Benet, 2005).

Variability in absorption of BCS class IV drugs is inherently problematic due to the relative impact that minor alterations in dissolution and permeability may have on the overall F_{oral} ; the low permeability and solubility makes it difficult to speculate on the impact of different factors on F_{oral} for this class (Wu and Benet, 2005).

As an extension to the BCS, Wu and Benet (2005) proposed the biopharmaceutics drug disposition classification system (BDDCS) replacing the permeability criteria with an elimination criteria, stating that a drug that exhibits $\geq 70\%$ metabolism will be highly permeable. The criteria defining BDDCS classification imply that biliary excretion potentially plays an important role in the disposition of class III and IV drugs due to the low level of metabolic elimination and predominantly renal elimination (Wu and Benet, 2005).

The evolution of predictive models provides a good starting point in identifying drug specific key parameters influencing oral drug bioavailability: Solubility, permeability, affinity to drug metabolising enzymes and active transporters.

Solubility

Although possible, it is cumbersome to measure drug dissolution *in vivo*, whereas *in silico* models for prediction of *in vivo* solubility from PhysChem properties (including: LogP, melting point, PSA and quantitative structure-activity relationships [QSAR]) display a high level of uncertainty where no single model provide a universal tool for predicting aqueous solubility (Bonlokke *et al.*, 2001; Dearden, 2006; Dressman *et al.*, 2007; Hewitt *et al.*, 2009). This leaves *in vitro* measurement as the most common source of solubility data.

The most relevant measurements of *in vitro* solubility in pharmaceutical R&D include the kinetic and equilibrium solubility methods. The determination of kinetic solubility involves the measurement of the maximum solubility of a compound's fastest precipitating species and is performed early in the drug discovery phase. The method may however over-predict the true solubility. Equilibrium solubility is determined by measuring the saturation solubility of a drug in equilibrium in an aqueous buffer using *e.g.* the shake-flask method (Elder and Holm, 2013).

Due to the many physiological factors that may impact dissolution *in vivo*, such as: surfactants, viscosity, pH, bile, food and fluid dynamics, the intrinsic solubility (solubility of the non-ionised species) in aqueous media may underestimate true solubility in the GI tract (Dressman and Reppas, 2000). To overcome the limitations of *in vitro* solubility studies, biorelevant dissolution media such as FaSSIF and FeSSIF (fasted and fed state simulated intestinal media respectively) have been developed to mimic *in vivo* conditions, thus potentially improving solubility estimates for highly lipophilic drugs displaying poor solubility in aqueous buffer (Dressman *et al.*, 2007; Fagerberg *et al.*, 2010). Current biorelevant dissolution media does however not account for the full complexity of human intestinal fluids, where considerable discrepancies in the apparent solubility have been identified. The utilisation of IVIVC to improve the predictability has been explored with successful findings but does however require further validation (Clarysse *et al.*, 2011; Wuyts *et al.*, 2013). An integrated approach utilising solubility data coupled with PBPK modelling and simulation provides a successful formula for validating dissolution media (Otsuka *et al.*, 2013).

Dissolution and formulation specific parameters

The dissolution rate (DR) of a given drug is governed by the surface area of a drug (A), the diffusion coefficient (D), the diffusion layer thickness (h), the saturation concentration of the drug in the GI tract (C_s), the amount dissolved (X_d) and the volume of the dissolution medium (V). The DR relation, originally developed by Noyes and Whitney (1897), and later refined by Nernst and Brunner in 1904, provides a theoretical framework for identifying formulation specific parameters, where C_s , A and h may be altered through changed formulation properties (Dokoumetzidis and Macheras, 2006). The most obvious formulation alterations include changes of particle size and wetting of a given drug to give an increase in

dissolution rate, through altering A (Noyes and Whitney, 1897; Dressman and Fleisher, 1986).

$$DR = \frac{A \cdot D}{h} \cdot \left(C_s - \frac{Xd}{V} \right)$$

Equation 1.4: Noyes-Whitney dissolution.

Numerous methods exist for enhancing solubilisation including the use of solutions, emulsions, microemulsions and micelles. Aqueous solutions can act to increase the solubility of hydrophobic drugs by utilising a pH buffer to increase the ionisation of weak acids and alkaline drugs or by the addition of a cosolvent or hydroxypropyl- β -cyclodextrins. Surfactants can be utilised to form a micelle forming emulsion, enhancing solubility by encapsulating the drug in micelles with a hydrophobic core and hydrophilic surface. Lipid microemulsions, such as cyclosporine Sandimmune Neoral (Sandoz), may improve solubilisation of a drug, reduce enzymatic hydrolysis and potentially improve permeability (Kovarik *et al.*, 1994; Constantinides, 1995; Narang *et al.*, 2007).

The design of a formulation is not always a consequence of poor solubility characteristics but can also be intended to provide an extended or controlled release (ER and CR respectively) in order to protect acid labile compounds (*e.g.* enteric-coating (EC)), or made to prolong the absorption phase of a given drug. The utilisation of ER formulations may have consequences on the f_a and F_G as absorption is delayed further distally to regions exhibiting a lower absorption capacity and abundance in drug metabolising enzymes (Sakr and Andheria, 2001; Wells and Losin, 2008).

Absorption

Following dissolution in the GI tract, an orally administered drug is subject to absorption. Permeability is highly relevant in determining the extent and rate of absorption of highly soluble low permeable (BCS class III) drugs. Human effective permeability ($P_{\text{eff, human}}$) has successfully been determined *in vivo* utilising jejunal perfusion (Loc-I-Gut) displaying excellent predictions of f_a in coupling with mechanistic modelling. The effective permeability represents the mass transfer of drug across the intestinal membrane as a function of perfusion

flow rate leaving the intestinal segment (Q_{out}), fluid-corrected concentrations entering and leaving the intestinal segment at steady state (C_{in} and C_{out}), and the surface area of the intestinal segment described as a cylinder (Lennernas *et al.*, 1992; Lennernas *et al.*, 1997).

$$P_{eff} = \frac{Q_{out} \cdot \left(\frac{C_{in} - C_{out}}{C_{out}} \right)}{2 \cdot \pi \cdot r \cdot L}$$

Equation 1.5: Determining P_{eff} *in vivo* utilising the jejunal perfusion technique (L=length, r=radius).

The Loc-I-Gut method is however difficult and costly to perform, thus leading to the utilisation of numerous different approaches to estimating permeability in human, including: *in vivo* animal models, *ex vivo* and *in situ* models in human and preclinical species, and *in vitro* methods coupled with IVIVC to obtain drug permeability parameters for human (Alqahtani *et al.*, 2013).

The Ussing chamber method utilises tissue samples from the intestine of preclinical species and human in order to determine apparent permeability (P_{app}) *ex vivo*. The method displays a good correlation with human f_a and allows the study of both passive and active transport across the epithelial membrane, thus allowing the study of transporter effects and regional differences in permeability. The method is however limited by its requirement for fresh tissue samples (Harwood *et al.*, 2013; Sjoberg *et al.*, 2013).

A number of *in vitro* assays are utilised to predict $P_{eff, human}$ which provide effective screening of drug specific permeability characteristics in pharmaceutical research. The most frequently utilised include: Caco-2 cell monolayers, Madin-Darby canine kidney (MDCK) cells and parallel artificial membrane assay (PAMPA).

The Caco-2 human colon adenocarcinoma cell line is highly utilised as a high-throughput screening method of intestinal drug permeability, allowing the study of passive transcellular, using for example transport inhibitors, and paracellular diffusion, and carrier-mediated transport across the epithelial membrane. The assay allows the determination of the effective or apparent permeability (P_{app}), as a flux per unit area over the cell monolayer based on the rate of drug appearance in the receiving compartment of the assay ($\Delta Q_R / \Delta t$), the area (A) and

the concentration of drug at time zero ($C_{D,0}$) (Equation 1.6) (Hidalgo *et al.*, 1989; Shah *et al.*, 2006; Sun *et al.*, 2008).

$$P_{app} = \frac{\Delta Q_R / \Delta t}{A \cdot C_{D,0}}$$

Equation 1.6: Apparent permeability (P_{app}).

This is based on a number of assumptions, including that the experiment is taking place under ‘sink condition’ and that accumulation of drug in the receiving compartment is proportional to time (Hidalgo *et al.*, 1989; Shah *et al.*, 2006; Sun *et al.*, 2008). IVIVC can be utilised to estimate $P_{eff, human}$ from Caco-2 monolayers where correlations have been developed based on the Loc-I-Gut method using calibration compounds (Equation 1.7) (Sun *et al.*, 2002).

$$\text{Log}P_{eff, human} = 0.6532 \cdot \text{Log}P_{app, Caco-2} - 0.3036$$

Equation 1.7: IVIVC between $P_{app, Caco-2}$ (pH 6.5) and $P_{eff, human}$.

Some of the drawbacks with the Caco-2 assay include: that it requires a long time to culture (~20 days); that it underestimates paracellular transport due to the tighter tight junctions expressed in its cultured cell monolayer compared to those *in vivo*; that it has an inherently low expression of CYP3A and that it displays high variability between laboratories (Shah *et al.*, 2006; Alqahtani *et al.*, 2013).

MDCK cell lines require a shorter culturing time (3-5 days) and are better predictors of paracellular transport. One of the disadvantages with this system is however that they are derived from canine kidney cells. MDCK cells transfected with human P-gp or MRP2 are commonly utilised to study transporter effects *in vitro* (Tang *et al.*, 2002a; Tang *et al.*, 2002b; Shah *et al.*, 2006). Similarly to Caco-2 cell lines, IVIVC has been developed for extrapolation to $P_{eff, human}$, where MDCK cell lines display good correlation with Caco-2 monolayers (Equation 1.8) (Irvine *et al.*, 1999; Gertz *et al.*, 2010).

$$\text{Log}P_{eff, human} = 0.829 \cdot \text{Log}P_{app, MDCK} - 1.30$$

Equation 1.8: IVIVC between $P_{app, MDCK-MDR1}$ and $P_{eff, human}$.

The PAMPA is a lipophilic artificial membrane allowing for rapid permeability screening without requiring cell culturing. The assay show good agreement of passive permeation and transcellular transport compared to Caco-2 monolayers and allows prediction of *in vivo* permeability using IVIVC (Equation 1.9) (Kansy *et al.*, 1998; Fujikawa *et al.*, 2005; Avdeef *et al.*, 2007; Gertz *et al.*, 2011).

$$\text{Log}P_{\text{eff, human}} = 0.6728 \cdot \text{Log}P_{\text{app, PAMPA}} - 0.0489$$

Equation 1.9: IVIVC between $P_{\text{app, PAMPA}}$ and $P_{\text{eff, human}}$.

Correlations have also been developed allowing the prediction of $P_{\text{eff, human}}$ from PhysChem descriptors such as the octanol/water distribution or partition coefficients (LogD or LogP) polar surface area (PSA) and HBD, where utilising LogD at a pH of 5.5 (LogD_{5.5}) together with PSA and HBD gave the best linear correlation ($R^2=0.93$). These models were however developed using a limited set of drugs (n drugs=13) (Winiwarter *et al.*, 1998).

$$\text{Log}P_{\text{eff, human}} = -2.883 - 0.010 \cdot \text{PSA} + 0.192 \cdot \text{Log}D_{5.5} - 0.239 \cdot \text{HBD}$$

Equation 1.10: Correlation between PhysChem descriptors and $P_{\text{eff, human}}$.

Metabolism

Drug specific affinities to metabolising enzymes, highly abundant in the small intestine and liver, play an important role in regulating F_{oral} . Numerous *in vitro* models are utilised in conjunction with IVIVE to determine drug metabolism in man, these include: primary hepatocytes, hepatoma cells, microsomes and precision-cut liver slice models; with human liver microsomes (HLM) being the most utilised system (Asha and Vidyavathi, 2010; Alqahtani *et al.*, 2013).

By measuring the rate of formation of metabolite or loss of substrate, enzyme kinetic analysis can be performed to determine the nonlinear saturable substrate concentration ([S]) dependent Michaelis-Menten kinetics of the metabolite formation, dependent on the parameters V_{max} (maximum velocity of the reaction) and K_m (the concentration that produces 50% of the maximal velocity). This provides an estimate of metabolic intrinsic clearance (Equation 1.11).

$$CL_{int} = \frac{V_{max} \cdot [S]}{K_m + [S]}$$

Equation 1.11: Michaelis-Menten elimination kinetics.

HLM are subcellular fractions prepared from human hepatocytes, and characteristically exhibit high levels of CYPs and UGTs. HLM can be utilised to identify and quantitatively assess metabolic pathways by introducing enzyme specific inhibitors. HLM have a number of advantages as being one of the most characterised *in vitro* systems to study metabolism and the possibility to study inter-individual variability (Asha and Vidyavathi, 2010; Alqahtani *et al.*, 2013).

Linear and nonlinear clearance estimations of a given enzyme (CYP_j) using HLM can be scaled to human using IVIVE, accounting for the fraction unbound of substrate in microsomes ($f_{u_{mic,j}}$), the abundance of enzyme *in vivo* ($A_{CYP,j}$) and the amount of microsomal protein (MP_i) per gram of liver (MPPGL) scaled to whole liver or microsomal protein per small intestine (MPPI) (Equation 1.2 and Equation 1.13) (Howgate *et al.*, 2006; Barter *et al.*, 2010).

$$CLu_{int} = \left[\sum_{j=1}^m \left(\frac{CL_{int}}{f_{u_{mic,j}}} \cdot A_{CYP,j} \right) \right] \cdot MP_i$$

Equation 1.12: IVIVE from CL_{int} in human liver microsomes to CLu_{int}.

$$CLu_{int} = \left[\sum_{j=1}^n \left(\frac{V_{max(CYP_j)} \cdot A_{CYP,j}}{K_{m,u(CYP_j)}} \right) \right] \cdot MP_i$$

Equation 1.13: IVIVE of Michaelis-Menten saturable enzyme kinetics from human liver microsomes to CLu_{int}.

Recombinant *in vitro* metabolism systems, such as baculovirus insect cells expressing recombinatory CYP450 (rCYP), has the advantage of offering enhanced assay sensitivity through artificially high enzyme expression levels. Recombinant systems require the

utilisation of a system and enzyme specific inter system expression factor (ISEF) in order to account for differences in enzyme activity (Stringer *et al.*, 2009).

$$CLu_{int} = \left[\sum_{j=1}^m \left(ISEF_j \cdot \frac{CL_{int}}{fu_{mic,j}} \cdot A_{CYP,j} \right) \right] \cdot MP_i$$

Equation 1.14: IVIVE from CL_{int} in human liver microsomes to CLu_{int} .

$$CLu_{int} = \left[\sum_{j=1}^n \left(\frac{ISEF_j \cdot V_{max(CYP_j)} \cdot A_{CYP,j}}{K_{m,u(CYP_j)}} \right) \right] \cdot MP_i$$

Equation 1.15: IVIVE of Michaelis-Menten saturable enzyme kinetics from recombinant P450 assays to CLu_{int} .

Hepatocytes offer the advantage of providing permeability limitation along with multi enzyme interactions as observed *in vivo* but used to require fresh liver tissue samples for preparation. Since the development of cryopreserved hepatocytes and cultured hepatocyte cell lines *in vitro* use of hepatocytes has gained new ground because of easier handling (Li, 2007).

Active transport

Depending on substrate specific affinity to intestinal transporters, a drug can be subject to altered bioavailability following oral administration; this can lead to either a reduction or increase in f_a depending on the transporters involved, and may give rise to nonlinear absorption kinetics depending on drug dissolution and permeability, as discussed above. As is the case for drug metabolising enzymes, active transport is a saturable process that can be described utilising Michaelis-Menten kinetics (Equation 1.16). Elucidating transporter kinetics does however require additional considerations as the drug is subject to passive diffusion clearance (CL_{PD}) across the membrane barrier (Harwood *et al.*, 2013).

$$CL_{int} = \frac{J_{max}}{K_m + C}$$

Equation 1.16: Michaelis-Menten transporter kinetics.

The determination of transporter kinetics *in vitro* and *ex vivo* uses many of the same methods utilised for permeability studies, namely: Caco-2, MDCK, Lilly Laboratory Cells – Porcine Kidney Nr. 1 (LLC-PK₁) assay and the Ussing chamber technique, where the transporter of interest may be expressed through transfection or be subjected to controlled inhibition in order to separate transporter effects from CL_{PD}. Transporter affinity can then be determined by measuring the bi-directional drug flux at a series of substrate concentrations. There are however issues regarding the IVIVE of transporter effects due to a number of disadvantages with current methods, including: the sparsity of quantitative absolute abundances of transporters *in vitro* and *in vivo* and the lack of transporter specific inhibitors. Due to this the extrapolation of transporter kinetics is done utilising relative expression factors (REF) based on the differences in expression utilising immunoblot densitometry *in vivo* compared to *in vitro* assays (Equation 1.17) (Harwood *et al.*, 2013).

$$REF = \frac{In\ vivo\ expression}{In\ vitro\ expression}$$

Equation 1.17: Relative expression factor (REF).

1.3 Physiologically-based pharmacokinetic modelling of oral drug bioavailability

Due to the sheer number of physiological, drug and formulation specific parameters and interrelations that determine the bioavailability of an orally administered drug, PBPK modelling and simulation lends itself well to create a framework for the prediction and extrapolation of absorption processes (Chow and Pang, 2013).

1.3.1 Modelling oral drug bioavailability

A constant evolution of PBPK modelling of oral drug bioavailability has occurred over the last decades where conceptually three approaches to describing absorption processes have emerged, namely: The mixing-tank model, dispersion models and compartmental transit models (Dokoumetzidis *et al.*, 2007).

The mixing-tank model considers the small intestine as a single compartment where a drug is administered as a bolus dose, subject to Noyes-Whitney dissolution and subsequent absorption or removal via small intestinal transit. As a result, the amount of dissolved drug will depend upon the amount available for dissolution (A_{undis}), its aqueous solubility (C_s), diffusion coefficient (D), particle density (ρ) and radius (r_i), the volume of the small intestinal lumen (V_{lumen}), the rate of absorption (k_a) and small intestinal transit (Q_{sit}) (Figure 1.1 and Equation 1.18) (Dressman and Fleisher, 1986).

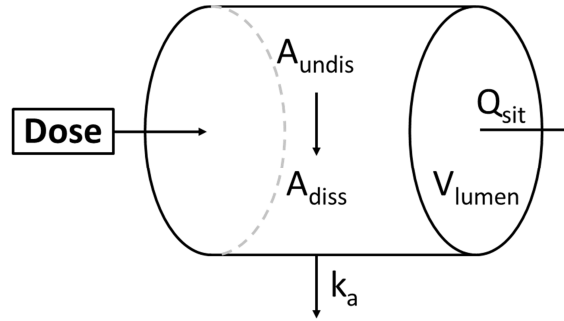


Figure 1.1. Schematics of the mixing tank model. A_{undis} =Amount undissolved drug, A_{diss} =Amount dissolved, k_a =Absorption rate constant, Q_{sit} =Small intestinal transit, V_{lumen} =Volume of small intestinal lumen. Adapted from Dressman and Fleisher (1986).

$$\frac{dA_{diss}}{dt} = \frac{3 \cdot D}{\rho \cdot h \cdot r_i} \cdot \left(Dose \cdot e^{-\frac{Q_{sit}(t)}{V_{lumen}}} \right)^{\frac{1}{3}} \cdot \left(C_s - \frac{A_{diss}}{V_{lumen}} \right) \cdot A_{undis}^{\frac{2}{3}} - k_a \cdot A_{diss} - \frac{Q_{sit} \cdot A_{diss}}{V_{lumen}}$$

Equation 1.18: Rate of change of amount dissolved described under the mixing tank model.

The dispersion model utilises partial differential equations to describe the intestine as a tube where drug concentration is described as a continuous profile over time subject to dispersion and transport along the small intestine. The model can be further refined to incorporate

spatial parameter variation to consider regional pH profiles, fluid dynamics, permeability and more, *e.g.* allowing the modelling of spatial luminal drug concentration (C_{lumen}) as a consequence of spatially varied transit (T_{SI}) and absorption (f_a), particle radius (r) and the length of the small intestine (L_{SI}) (Figure 1.2 and Equation 1.19) (Willmann *et al.*, 2003; Willmann *et al.*, 2004; Dokoumetzidis *et al.*, 2007).

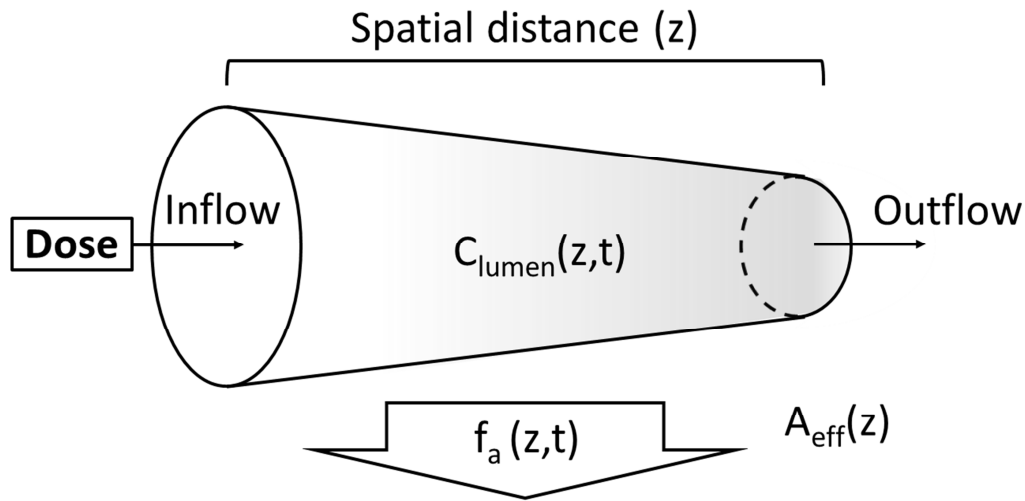


Figure 1.2. Conceptual schematic of the dispersion model of oral drug absorption.

C_{lumen} =Spatially varied time dependent luminal drug concentration, f_a =absorption,

A_{eff} =Effective permeability. Adapted from Willmann *et al.*, (2004) and Dokoumetzidis *et al.*, (2007).

$$\frac{\partial C_{\text{lumen}}(z, t)}{\partial t} = \frac{\text{Dose} \cdot [1 - f_a(z, t)]}{\pi \cdot r^2 \cdot L_{\text{SI}}} \cdot T_{\text{SI}}(z, t)$$

Equation 1.19: Conceptual partial differential equation for dispersion absorption model.

The compartmental absorption and transit (CAT) model, developed by Yu and Amidon (1999), utilises an equally divided seven compartment absorption model to describe the amount of drug (A_n) subject to small intestinal transit (k_{sit}) providing a flexible and more mechanistic description of the processes of intestinal transit as compared to the single-compartment absorption model and a reduced complexity of implementation compared to the dispersion model (Yu *et al.*, 1996; Yu and Amidon, 1999).

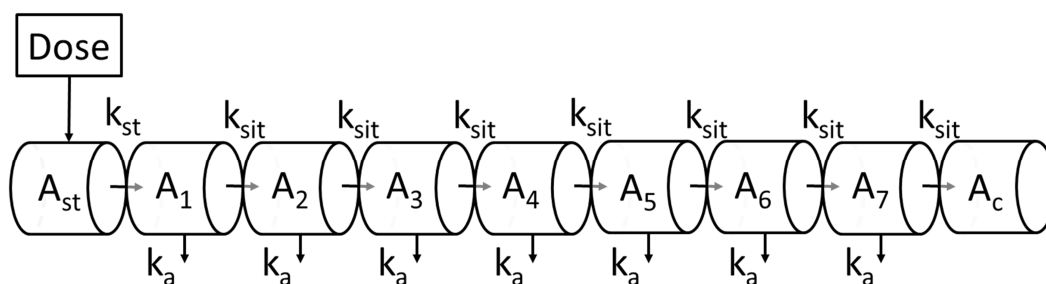


Figure 1.3. Schematic of the nine segment compartmental absorption model (CAT) model. A_{st} =Amount of drug in the stomach, A_n =Amount of drug in the n th small intestinal compartment, A_c =Amount of drug in the colon, k_{st} =Gastric emptying rate, k_{sit} =Small intestinal transit rate and k_a =Absorption rate constant. Adapted from Yu and Amidon (1999).

The CAT model serves as the basis for some of the most physiologically sophisticated PBPK models for oral drug bioavailability, including the implementations of the advanced compartmental absorption and transit (ACAT) and advanced dissolution absorption and metabolism (ADAM) models, incorporated into GastroPlus and the Simcyp Simulator respectively (Figure 1.4). These models further expand on the CAT model by adapting gastrointestinal compartments to conform to their physiological counterparts (*i.e.* the stomach, duodenum, jejunum, ileum and colon) with corresponding fluid volumes ($V_{lumen,n}$), transit times based on segment length (kt_n), regional distribution of enzymes and transporters, segmented segregated blood flows. The drug-related components of the model are refined to incorporate formulation subject to release, dissolution, supersaturation, and precipitation, absorption, active transport and metabolism in the enterocytes. In addition, the ADAM model incorporates inter-individual variability in physiological parameters (Agoram *et al.*, 2001; Jamei *et al.*, 2009).

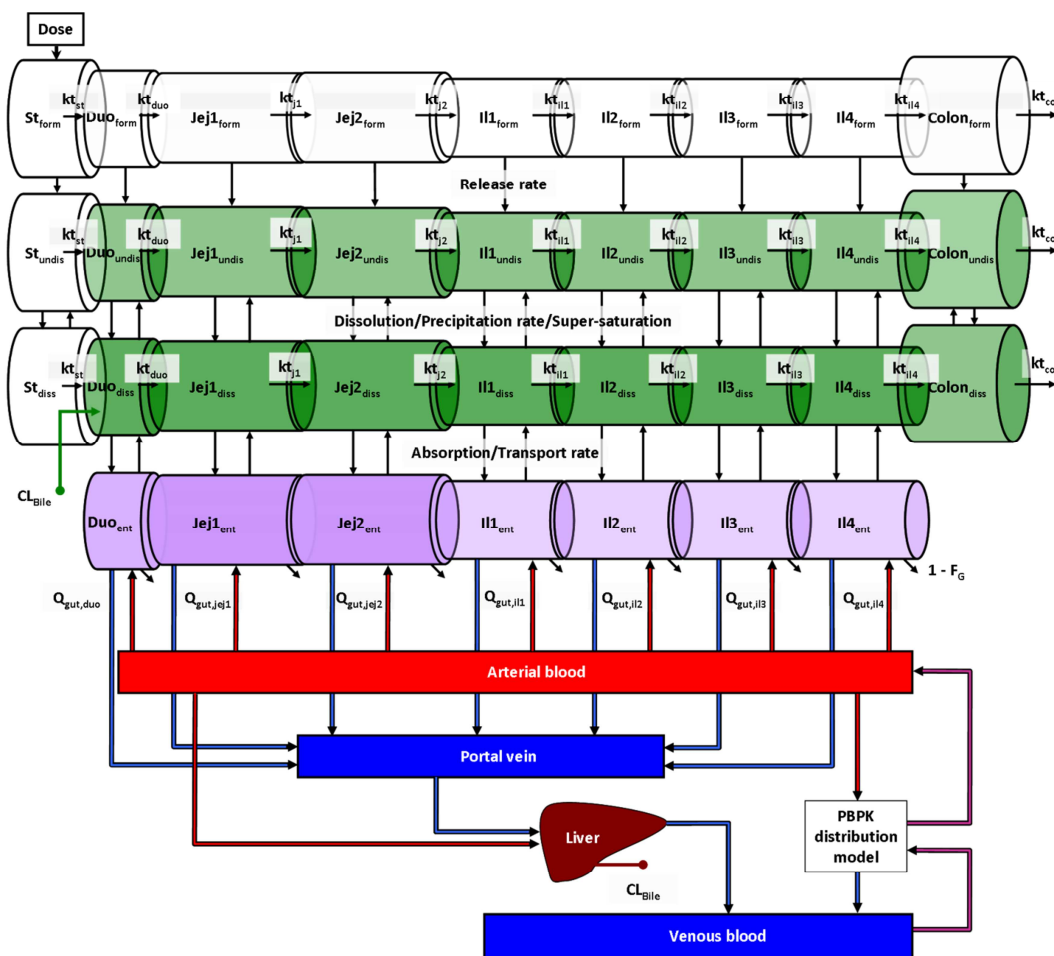


Figure 1.4. Depiction of the 9 segment ADAM model, consisting of following compartments: Stomach, Duodenum, Jejunum I, Jejunum II, Ileum I-IV, and Colon. Further describing: St=stomach, Jej1 & 2=jejunum, Il1-4=ileum, form=drug trapped in formulation, undiss=undissolved drug, diss= dissolved drug, ent=fraction absorbed drug in enterocytes, kt_n =transit rate, Q_n =gastrointestinal blood flow, F_G =fraction drug that escapes gut wall metabolism, CL_{bile} =biliary clearance. Compartment size and purple colour intensity (■) refers to segmental length and regional abundance of CYP3A4 respectively. Green colour scheme (■) indicates bile enhanced solubility. Adapted from Jamei, and co-workers (2009).

PBPK modelling of GI drug release and dissolution utilises a large set of models to describe the dissolution profile time course of amount dissolved, including: zero, first and second order models, Higuchi zero order and more. One of the most frequently utilised models is an adaptation of the empirical Weibull distribution allowing it to conform to most release and dissolution profiles by estimating scale and shape parameters α and β , and the lag time prior

to release (T_{lag}), giving the accumulated release (m) over time (t) (Equation 1.20) (Langenbucher, 1972; Costa and Sousa Lobo, 2001).

$$m = 1 - \exp \left[\frac{-(t - T_{lag})^\beta}{\alpha} \right]$$

Equation 1.20: Weibull function for dissolution profiles.

Where dissolution profiles are lacking, the pH dependent solubility of a drug is obtained either through the Henderson-Hasselbalch equation or preferably using interpolation of experimentally derived solubility data at GI pH range (Bergstrom *et al.*, 2004). The solubility of a given drug in the GI tract is modelled utilising the diffusion layer models for solid dissolution developed by Noyes and Whitney (1897) or modified versions, such as the Nernst and Brunner equation which consider the dissolution from a planar surface (Dokoumetzidis and Macheras, 2006). Additional modifications of the diffusion layer model allow the modelling of dissolution of spherical mono-dispersed particles under sink and non-sink conditions, where equilibrium between the amount of dissolved ($A_{diss,n}$) and undissolved compound ($A_{undis,n}$) is dependent upon pH dependent solubility at the particle surface ($C_{s,n}$), the luminal volume ($V_{lumen,n}$), particle radius (r), density (ρ), diffusion coefficient (D) and diffusion layer thickness (h), as the drug is subject to transit (kt_n) through the GI tract and first order rate absorption of dissolved drug ($k_{a,n}$) (Equation 1.21 and Equation 1.22) (Wang and Flanagan, 1999; Wang and Flanagan, 2002; Jamei *et al.*, 2009; Gertz *et al.*, 2011).

$$\frac{dA_{undis,n}}{dt} = A_{undis,n-1} \cdot kt_{n-1} - A_{undis,n} \cdot kt_n - \frac{3 \cdot D}{\rho \cdot r \cdot h} \cdot A_{undis,n} \cdot \left(C_{s,n} - \frac{A_{dis,n}}{V_{lumen,n}} \right)$$

Equation 1.21: Rate of change of amount undissolved drug in the gut lumen.

$$\begin{aligned} \frac{dA_{diss,n}}{dt} = & A_{diss,n-1} \cdot kt_{n-1} + \frac{3 \cdot D}{\rho \cdot r \cdot h} \cdot A_{undis,n} \cdot \left(C_{s,n} - \frac{A_{diss,n}}{V_{lumen,n}} \right) \\ & - A_{diss,n} \cdot kt_n - A_{diss,n} \cdot k_{a,n} \end{aligned}$$

Equation 1.22: Rate of change of amount dissolved drug in the gut lumen.

The luminal volume in the stomach (V_{st}) and intestine ($V_{lumen,n}$) is either assumed to be a constant segmented volume, as in the ACAT model, or as a dynamic system based on physiological data on secretion of intestinal fluids in the stomach and small intestine ($Q_{sec,n}$) subject to reabsorption ($k_{reabs,n}$), gastric emptying ($k_{t,st}$) and transit ($k_{t,n}$) throughout the GI tract (Equation 1.23 and Equation 1.24) (Jamei *et al.*, 2009; Sutton, 2009).

$$\frac{dV_{st}}{dt} = Q_{sec,s} - k_{t,st} \cdot V_{st}$$

Equation 1.23: Gastric fluid dynamics.

$$\frac{dV_{lumen,n}}{dt} = Q_{sec,n} - k_{reabs,n} \cdot V_{lumen,n} + k_{t,n-1} \cdot V_{lumen,n-1} - k_{t,n} \cdot V_{lumen,n}$$

Equation 1.24: Intestinal fluid dynamics.

The solubility of drug in bile micelle media (S_{diss}) can be modelled utilising the modified Henderson-Hasselbalch equation, as a function of the concentration of bile (C_{bile}) compared to water (C_{H_2O}), the drug specific micelle aqueous partition coefficient for the neutral drug ($K_{bm,0}$), K_{bm} for the ionised base or acid ($K_{bm,+}$ or $K_{bm,-}$), the hydrogen ion concentration $[H^+]$ and the equilibrium constant for the ionisation (K_a); where K_{bm} can be derived from $\text{Log}P_{o:w}$ (Equation 1.25, Equation 1.26, Equation 1.27, Equation 1.28 and Equation 1.29) (Rippie *et al.*, 1964; Jinno *et al.*, 2000; Sugano, 2009).

$$S_{diss} = S_0 \cdot \left(1 + \frac{[H^+]}{K_a} + \frac{C_{bile}}{C_{H_2O}} \cdot K_{bm,0} + \frac{[H^+]}{K_a} + \frac{C_{bile}}{C_{H_2O}} \cdot K_{bm,+} \right)$$

Equation 1.25: Bile enhanced solubilisation of an alkaline compound.

$$S_{diss} = S_0 \cdot \left(1 + \frac{K_a}{[H^+]} + \frac{C_{bile}}{C_{H_2O}} \cdot K_{bm,0} + \frac{K_a}{[H^+]} + \frac{C_{bile}}{C_{H_2O}} \cdot K_{bm,-} \right)$$

Equation 1.26: Bile enhanced solubilisation of an acidic compound.

$$\text{Log}K_{bm,0} = 0.74 \cdot \text{Log}P_{o:w} + 2.29$$

Equation 1.27: Micelle aqueous partition coefficient for a neutral drug.

$$\text{Log}K_{bm,+} \approx \text{Log}K_{bm,o} - 1$$

Equation 1.28: Micelle aqueous partition coefficient for an ionised base.

$$\text{Log}K_{bm,-} \approx \text{Log}K_{bm,o} - 2$$

Equation 1.29: Micelle aqueous partition coefficient for an ionised acid.

Oral absorption

In the absence of active transport, absorption is modelled as a concentration dependent first order process, governed by a rate constant ($k_{a,n}$) proportional to the $P_{\text{eff,human}}$ considering the small intestinal radius ($r_{\text{si},n}$) (Equation 1.30). Absorption from different segments of the intestine can be considered by changing $r_{\text{si},n}$ to the corresponding physiological value (Sinko *et al.*, 1991; Yu and Amidon, 1999).

$$k_{a,n} = \frac{2 \cdot P_{\text{eff}}}{r_{\text{si},n}}$$

Equation 1.30: Estimate of absorption rate constant from P_{eff} .

Gut-wall metabolism

Gut-wall metabolism can be incorporated into the model of the concentration of substrate in a well-stirred enterocyte compartment. The overall concentration of drug in the enterocytes ($C_{\text{ent},n}$) will depend on $k_{a,n}$, the fraction unbound ($fu_{\text{ent},n}$), the amount of active enzyme in the small intestine ($A_{\text{Enz},n}$), the blood flow out of the enterocytes to the portal vein ($Q_{\text{Gut},n}$), as well as the drug specific clearance parameters (V_{max} and K_m) giving rise to the net $CL_{\text{u,int}}$ (Equation 1.31) (Jamei *et al.*, 2009; Gertz *et al.*, 2011).

$$V_{\text{ent},n} \cdot \frac{dC_{\text{ent},n}}{dt} = k_{a,n} \cdot A_{\text{diss},n} - \frac{V_{\text{max}} \cdot A_{\text{Enz},n} \cdot fu_{\text{ent},n} \cdot C_{\text{ent},n}}{K_m + fu_{\text{ent},n} \cdot C_{\text{ent},n}} - fu_{\text{ent},n} \cdot C_{\text{ent},n} \cdot CL_{\text{u,int,GI}} - Q_{\text{Gut},n} \cdot C_{\text{ent},n}$$

Equation 1.31: Model for rate of change of drug concentration in enterocytes, incorporating gut wall metabolism.

Nonlinear active efflux from the enterocytes to the intestinal lumen can be incorporated into the enterocyte model as well, described in a similar fashion to metabolic clearance utilising Michaelis-Menten kinetics where the outflow of the clearance term goes to dissolved drug in the intestinal lumen (Darwich *et al.*, 2010).

Hepatic clearance

Hepatic first-pass elimination can be modelled using a well-stirred model for the liver compartment where the elimination of drug will depend on the unbound concentration of drug in liver ($f_{ub} \cdot C_{hep}$). Assuming a perfusion limited liver, the concentration of drug in the liver also depends on inflow of drug from the intestine ($Q_{gut,1:n}$) and the systemic influx via the hepatic artery (Q_{HA}) and an outflow equal to the sums of the inflow (Equation 1.32) (Rowland Yeo *et al.*, 2010; Pertinez *et al.*, 2013). Additional models for the liver exist in order to accommodate active hepatic uptake, such as the dispersion model (Roberts and Rowland, 1986; Yang *et al.*, 2007a).

$$V_{hep} \cdot \frac{dC_{hep}}{dt} = Q_{Gut,1:n} \cdot C_{ent,1:n} + Q_{HA} \cdot C_{sys} - C_{hep} \cdot (f_{ub} \cdot CL_{u_{int,H}} + Q_{Gut,1:n} + Q_{HA})$$

Equation 1.32: The well-stirred perfusion-limited liver model.

Hepatobiliary elimination

Hepatobiliary clearance can be modelled either as a clearance from vascular liver compartment (CL_{bile}) to the duodenum or utilising Michaelis-Menten transporter kinetics to account for observed nonlinearity due to the transporter mediated clearance from the sinusoidal side of the liver. Because of the sequential nature of biliary secretion into the small intestine the utilisation of transit compartments or time-to-event modelling may be necessary to account for double peak phenomena (Bischoff *et al.*, 1971; Hofmann *et al.*, 1983).

1.3.2 Whole-body distribution

Distribution is defined as the reversible transfer of drug between different tissues of the body. The distribution of a drug can be modelled empirically by estimating inter-compartmental clearances and volumes of systemic blood or plasma and peripheral compartments (Rowland and Tozer, 1989).

A more mechanistic approach to modelling distribution is to describe drug concentrations in physiological tissues ($C_{T,n}$), compared to venous blood or plasma (C_v), resulting in the tissue to plasma partition coefficient ($K_p = C_{T,n}/C_v$). Direct measurements of K_p are often however lacking in man and rely instead on the utilisation of data from preclinical species or extrapolation from *in vitro* and PhysChem parameters. Utilising K_p s, the plasma volume of distribution at steady state following iv infusion (V_{ss}) can be estimated from the volumes of individual tissues (V_t) and plasma (V_p) (Equation 1.33) (Graham *et al.*, 2012).

$$V_{ss} = \sum (K_p \cdot V_t) + V_p$$

Equation 1.33: Estimate of volume of distribution.

Mechanistic methods for estimating human K_p values from *in vitro* data to man include the equations developed by Poulin and Theil (2000), where K_p values can be estimated the olive oil buffer distribution coefficient at pH 7.4 ($K_{vo:w}$), tissue volumes (V), fractional tissue volumes of phospholipids (ph), neutral lipids (nl), water (w) in tissue (t) and plasma (p), the fraction unbound in plasma ($f_{u,p}$) and tissue ($f_{u,t}$) for estimates of K_p values in non-adipose ($K_{p,t}$) and adipose tissues ($K_{p,adi}$) (Equation 1.34 and Equation 1.35 respectively) (Poulin and Theil, 2000; Poulin and Theil, 2002b; Poulin and Theil, 2002a). Refined models based on the Poulin and Theil model have been developed to allow better predictions of highly lipophilic drugs (Berezhkovskiy, 2004; Poulin and Haddad, 2012).

$$K_{p,t} = \frac{[K_{vo:w} \cdot (V_{n,t} + 0.3 \cdot V_{ph,t})] \cdot [(V_{w,t} + 0.7 \cdot V_{ph,t})]}{[K_{vo:w} \cdot (V_{n,p} + 0.3 \cdot V_{ph,p})] \cdot [(V_{w,p} + 0.7 \cdot V_{ph,p})]} \cdot \frac{f_{u,p}}{f_{u,t}}$$

Equation 1.34: Poulin and Theil model for estimating K_p .

$$K_{p,adi} = \frac{[K_{vo:w}^* \cdot (V_{n,t} + 0.3 \cdot V_{ph,t})] \cdot [(V_{w,t} + 0.7 \cdot V_{ph,t})]}{[K_{vo:w}^* \cdot (V_{n,p} + 0.3 \cdot V_{ph,p})] \cdot [(V_{w,p} + 0.7 \cdot V_{ph,p})]} \cdot \frac{f_{u,p}}{1}$$

Equation 1.35: Poulin and Theil model for estimating $K_{p,adi}$.

In addition to the Poulin and Theil derived models, an alternative model by Rodgers *et al.* (2005) has been proposed for the prediction of unbound K_p values ($K_{pu} = K_p/f_{u,p}$). The

Rodgers and Rowland model separates intra- and extracellular volumes as fractions (f_{IW} and f_{EW}) and takes the ion species of the compound and pH dependent ionisation into account. One model is utilised for moderate to strong bases, requiring the association constant (Ka) with concentration of acidic phospholipid ($[AP^-]$) and P to predict Kpu values. A separate model is used for neutral, acid, weak alkaline and zwitterions, taking the concentration of binding protein in the tissue and plasma into account ($[PR]_T$ and $[PR]_P$ respectively) assuming only unionised unbound drug permeates into tissues, and specifying the permeation species (Y) dependent on the compound's acid-base nature (Rodgers *et al.*, 2005; Rodgers and Rowland, 2006; Rodgers and Rowland, 2007).

$$Kpu = \left[f_{EW} + \left(\frac{1 + 10^{pKa-pH_{IW}}}{1 + 10^{pKa-pH_p}} \cdot f_{IW} \right) + \left(\frac{Ka \cdot [AP^-]_T \cdot 10^{pKa-pH_{IW}}}{1 + 10^{pKa-pH_p}} \right) + \left(\frac{(P \cdot f_{NL} + ((0.3 \cdot P + 0.7) \cdot f_{NP}))}{1 + 10^{pKa-pH_p}} \right) \right]$$

Equation 1.36: Rodgers and Rowland model for estimating Kp 's of moderate to strong bases.

$$Kpu = \frac{X \cdot f_{IW}}{Y} + f_{EW} + \left(\frac{P \cdot f_{NL} + (0.3 \cdot P + 0.7) \cdot f_{NP}}{Y} \right) + \left[\left(\frac{1}{f_u} - 1 - \left(\frac{P \cdot f_{NL,P} + (0.3 \cdot P + 0.7) \cdot f_{NP,P}}{Y} \right) \right) \cdot \frac{[PR]_T}{[PR]_P} \right]$$

Equation 1.37: Rodgers and Rowland model for estimating Kp 's of neutral, acid, weak alkaline and zwitterions compounds.

The Rodgers and Rowland model displays improved predictions for compounds compared to the Poulin and Theil method for specific different drug classes and tissues, whereas Poulin and Theil displays a higher accuracy for the prediction of V_{ss} (Graham *et al.*, 2012).

Observed or predicted Kp values can be utilised in whole-body PBPK tissue distribution models to model and predict venous, arterial and tissue concentrations, where the tissue

concentration (C_T) in a well-perfused tissue will depend on the tissue specific blood flow (Q_T), volume (V_T) and K_p (Figure 1.5 and Equation 1.38) (Nestorov *et al.*, 1998).

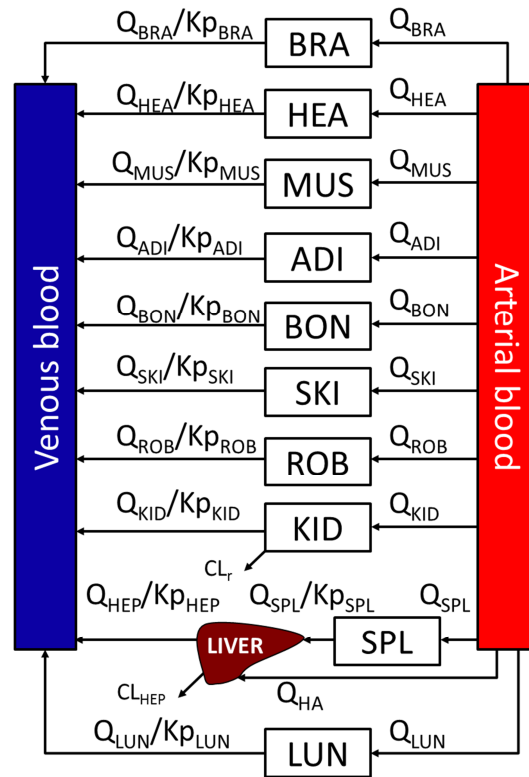


Figure 1.5. Whole-body distribution model describing the partitioning of drugs into tissues as compared to blood (K_{p_n}) dependent upon tissue specific blood flows (Q_n) and volumes (V_n). BRA=Brain, HEA=Heart, MUS=Muscle, ADI=Adipose, BON=Bone, SKI=Skin, ROB=Rest of body, KID=Kidney, SPL=Splanchnic organs, LUN=Lungs, CL_r =Renal clearance and CL_{HEP} =Hepatic clearance. Adapted from Nestorov *et al.*, (1998).

$$\frac{dC_T}{dt} = \frac{Q_T}{V_T} \cdot C_{ART} - \frac{Q_T}{V_T \cdot K_P} \cdot C_T$$

Equation 1.38: Modelling tissue disposition in well-perfused non-eliminating tissues.

1.3.3 Modelling metabolic drug-drug interactions in the small intestine

PBPK M&S is a highly utilised approach for the implementing mechanistic prediction of metabolic enzyme DDIs, enabling the utilisation of drug specific inhibitory and induction parameters from *in vitro* assays, such as HLM and hepatocytes. In addition to the static models a PBPK M&S approach may show improved predictions as well as incorporate inter-individual variability to aid the prediction of DDIs (Fahmi *et al.*, 2009). The food and drug administration (FDA) has recognised the utilisation of PBPK modelling and simulation as a useful tool to quantitatively predict the impact of DDIs and assist the design of DDI studies (Rostami-Hodjegan, 2012).

The potency of a reversible enzyme inhibitor, including competitive and non-competitive inhibitors, can be established *in vitro* by determining the unbound inhibition constant ($K_{i,u}$), where the fold reduction in $CL_{u,int}$ following inhibition is dependent on the concentration of the inhibitor and $K_{i,u}$ (Equation 1.39) (Rostami-Hodjegan and Tucker, 2004).

$$\text{Fold reduction in } CL_{u,int,GI} = \left(1 + \frac{[I]}{K_{i,u}} \right)$$

Equation 1.39: Impact on substrate clearance following reversible enzyme inhibition.

Mechanism-based inhibition (MBI) is characterised by the time-dependent inhibition of the level of active enzyme. Utilising *in vitro* metabolic assays the maximum rate of enzyme inactivation (k_{inact}) and unbound dissociation constant ($K_{I,u}$) can be determined and used to predict the level of enzyme inactivation over time. The net rate of inactivation will further depend on unbound inhibitor concentration in the gut ($fu_{Gut} \cdot [I]_{GI}$) and the baseline turnover of the enzyme ($k_{deg,GI}$) (Equation 1.40). Issues do however exist regarding the prediction of MBIs where over-predictions of the level of enzyme inhibition have been reported (Rostami-Hodjegan and Tucker, 2004; Obach *et al.*, 2007; Ohno *et al.*, 2008; Obach, 2013).

$$\frac{dA_{Enz,GI}}{dt} = R_{Syn-Enz,GI} - A_{Enz,GI} \cdot \left(k_{deg,GI} + \frac{k_{inact} \cdot fu_{Gut} \cdot [I]_{GI}}{K_{I,u} + fu_{Gut} \cdot [I]_{GI}} \right)$$

Equation 1.40: Amount of active enzyme in GI tract with over time following MBI - R_{syn} =base rate of synthesis.

Enzyme induction can be modelled utilising a Hill function, dependent on the maximum induction effect (E_{max}), 50% maximal induction effect ($EC_{50,I}$), the unbound inhibitor concentration in the enterocytes ($fu_{Gut} \cdot [I]_{GI}$) and enzyme turnover in the gut ($k_{deg,GI}$) (Equation 1.41) (Ohno *et al.*, 2008; Guo *et al.*, 2013).

$$\frac{dA_{Enz,GI}}{dt} = R_{Syn-Enz,GI} \cdot \left(1 + \frac{E_{max} \cdot fu_{Gut} \cdot [I]_{GI}}{fu_{Gut} \cdot [I]_{GI} + EC_{50,I}} \right) - k_{deg,GI} \cdot A_{Enz,GI}$$

Equation 1.41: Amount of active enzyme in GI tract over time following induction.

Instances where induction is accompanied by MBI, such as for ritonavir, requires PBPK modelling and simulation due to the complexity of the interaction, which must combine the processes described in Equation 1.40 and Equation 1.41 in a single scheme (Fahmi *et al.*, 2008; Ohno *et al.*, 2008).

1.3.4 Mechanistic modelling of special subpopulations

PBPK M&S and system pharmacology provides a framework for modelling drug exposure in special disease subpopulations due to its inherent ability to facilitate extrapolation by using physiology and anatomy to inform compartmental models. By utilising a systems pharmacology approach predictive models become attractive for special subpopulations that are not readily available for clinical research due to ethical or practical considerations. A number of special population PBPK models have been developed utilising this approach, including those for: Paediatrics, pregnancy, liver cirrhosis, renal failure, obesity as well as genetic differences in enzyme expression (Barter *et al.*, 2010; Johnson *et al.*, 2010; Ghobadi *et al.*, 2011; Johnson and Rostami-Hodjegan, 2011; Rowland Yeo *et al.*, 2011; Ke *et al.*, 2012).

The utilisation of PBPK M&S together with IVIVE/C under the paradigm of systems pharmacology (together with the increased acceptance from the regulatory agencies for the utilisation of PBPK M&S in submission process and the emergence of individualised pharmacotherapy), in development of new mechanistic models for special subpopulation. The approach allows the assessment and prediction of (amongst others): study design issues and the powering of studies, the impact of enzyme ontogeny on metabolic clearance in

paediatrics, and the effect of expected variability in drug exposure in special populations (Zhao *et al.*, 2011; Rostami-Hodjegan, 2012).

The general method for the development of PBPK models for special subpopulations relies heavily on identification and extraction of multidisciplinary information relating to the alterations in physiological system specific parameters, coupled with statistical meta-analysis in order to estimate the variability of these system-specific parameters in the subpopulation in question. This specialised information regarding the physiological parameters of the subpopulation is needed in addition to an appropriate level of drug specific information in order carry out informative extrapolation within a general framework for PBPK modelling and model validation. The approach is very data intense and may therefore be limited in application to well-characterised subpopulations, with drugs which can be considered to show the greatest challenges in extrapolation between populations and for which there is knowledge of the impact of population covariates on drug disposition. An additional obstacle is the need for best practice guidelines in order to streamline the development process (Zhao *et al.*, 2011).

1.3.5 Bariatric surgery subpopulation

The number of bariatric surgical procedures carried out in North America and the United Kingdom has increased dramatically in recent years. The rise in surgical procedures can be attributed to the increased prevalence of obesity and the proven clinical and cost effectiveness of surgical treatment of obesity and associated comorbidities (Picot *et al.*, 2009; Flegal *et al.*, 2010; OHE, 2010). Several bariatric surgical procedures exist in healthcare varying in degree of invasiveness. Procedures such as the sleeve gastrectomy are limited to restricting the capacity of the gastric pouch whereas procedures as the Roux-en-Y gastric bypass and biliopancreatic diversion with duodenal switch result in gastric resection, small intestinal bypass and delay in bile inlet. These surgical procedures will result in a number of GI anatomical and physiological alterations, where they for example may alter the gastric volume, pH, gastric emptying, GI fluid dynamics, absorption area, and exposure to gut-wall enzymes and transporters (Behrns *et al.*, 1994; Buchwald and Oien, 2009).

Potential anatomical and physiological changes following bariatric surgery have clear implications on the exposure of orally administered drugs and consequently the

pharmacotherapy in a post bariatric surgery population. Clinical evidence suggests trends in oral drug exposure pre to post bariatric surgery to be highly variable, both drug and surgery dependent. This presents an apparent problem in the pharmacological treatment of post bariatric surgery patients where clinical data, and guidance on appropriate drug utilisation is lacking (Padwal *et al.*, 2009; Skottheim *et al.*, 2009; Skottheim *et al.*, 2010).

Due to the multi-factorial changes in the GI physiology and anatomy, a systems pharmacology PBPK approach may be particularly suitable approach for exploring the underlying processes resulting in alterations of oral drug exposure and may also inform clinical pharmacology in the treatment of post bariatric surgery patient populations.

1.4 Project aims and objectives

The aim of the work constituting this thesis was to examine the interplay between gastrointestinal systems parameters and their effects on oral drug bioavailability utilising physiologically-based pharmacokinetic modelling and simulation under a systems pharmacology approach.

The research would be carried out with the focus on PBPK M&S of trends in oral drug bioavailability in pre to post bariatric surgery subpopulation, resulting in the partial resection of the GI tract, in order to enable the theoretical examination of underlying physiological, drug and formulation specific factors accounting for observed changes in oral drug exposure pre to post surgery.

In order to establish the current knowledge around changes in oral drug exposure following bariatric surgery a systematic review of the topic would be performed together with surveying the clinical pharmacotherapeutical considerations at an NHS (National Health Services) hospital.

The review would be followed by characterisation of relevant systems parameters in a post bariatric surgery patient subpopulation in order to enable the PBPK model development and assessment utilising the Simcyp Simulator ADAM model. Developed models would then be subject to validation against observed clinical data.

The work in this thesis would also theoretically examine the nested turnover of CYP enzymes dependent on the turnover of the enterocytes and its impact on the prediction of mechanism-based enzyme inhibition in the small intestine. This would be carried out through characterising systems parameters relating to enterocyte and enzyme turnover that would be incorporated into a nested enzyme-within-enterocyte (NEWE) PBPK model. The discrepancies in the NEWE model predictions of mechanism-based inhibition would then be assessed against the conventional modelling approach only considering a lumped enzyme turnover in the gut.

The work would be carried out under the principles of the systems pharmacology approach, incorporating IVIVE, IVIVC, and statistical meta-analysis coupled with physiologically-based pharmacokinetic modelling and simulation in the development and assessment of mechanistic PBPK models for oral drug bioavailability.

1.5 List of manuscripts and author contribution statement

In accordance with University of Manchester guidelines for the alternative thesis format for doctor in philosophy, beneath follows a statement of the individual contributions of authors to published manuscripts and manuscripts in preparation. Please note that published manuscripts, Chapter 2-4, are available in their respective appendices.

Chapter 2:

Br J Clin Pharmacol. 2012,74(5):774-87

Trends in oral drug bioavailability following bariatric surgery: examining the variable extent of impact on exposure of different drug classes

A.S. Darwich: Literature search, data and statistical analysis, study design and lead coordination of clinical audit study design and execution, supervision of research carried out by K. Henderson, main preparation of manuscript.

K. Henderson: Literature search, data collection for clinical audit, preliminary data analysis. Preparation of manuscript, mainly clinical audit section. Please note that parts of the clinical audit sections in the published manuscript and as provided in this thesis is therefore available in the project report (titled: ‘An investigation into trends in altered bioavailability following

gastric bypass surgery') by K. Henderson, as supervised and edited by A.S. Darwich and A. Rostami-Hodjegan. The work was carried out as a part of Master of Pharmacy project report.

A. Burgin: Supervision of K. Henderson during clinical audit, coordination of data collection during the clinical audit and input on manuscript.

N. Ward: Expert opinion on clinical pharmacotherapy following bariatric surgery and input on manuscript.

J. Whittam: Expert opinion on clinical pharmacotherapy following bariatric surgery, input on clinical audit study design and manuscript.

B.J. Ammori: Expert opinion on bariatric surgical procedures, input on manuscript.

D.M. Ashcroft: Supervision of research, study design, preparation of manuscript.

A. Rostami-Hodjegan: Supervision of research, study design, input on data analysis, preparation of manuscript.

Chapter 3:

J Pharm Pharmacol. 2012, 64(7):1008-24

A mechanistic pharmacokinetic model to assess modified oral drug bioavailability post bariatric surgery in morbidly obese patients: interplay between CYP3A gut wall metabolism, permeability and dissolution

A.S. Darwich: Lead for study design, literature search and meta-analysis, modelling and simulation of post bariatric surgery models, data analysis and preparation of manuscript.

D. Pade: Input on model development and manuscript.

B.J. Ammori: Expert opinion on bariatric surgical procedures, input on surgical dimensions in models for post bariatric surgery populations and manuscript.

M. Jamei: Expert opinion and input on PBPK modelling, and input on manuscript.

D.M. Ashcroft: Supervision of research, study design and input on manuscript.

A. Rostami-Hodjegan: Supervision of research, study design, input on modelling and simulation of post bariatric surgery models and input on manuscript.

Chapter 4:

CPT Pharmacometrics and Syst Pharmacol. 2013, 2(e47):1-9

Evaluation of an *in silico* PBPK post-bariatric surgery model through simulating oral drug bioavailability of atorvastatin and cyclosporine

A.S. Darwich: Lead for study design, modelling and simulation utilising post bariatric surgery PBPK models, data analysis and preparation of manuscript.

D. Pade: Input on model development and simulation, and manuscript.

K. Rowland-Yeo: Input on modelling of atorvastatin acid and manuscript.

M. Jamei: Expert opinion and input on PBPK modelling, and input on manuscript.

A. Åsberg: Supply of atorvastatin data and input on PBPK modelling and manuscript.

H. Christensen: Supply of atorvastatin data and input on modelling and manuscript.

D.M. Ashcroft: Supervision of research, study design and input on manuscript.

A. Rostami-Hodjegan: Supervision of research, study design, input on PBPK modelling and simulation, and input on manuscript.

Chapter 5:

In preparation

Assessing the turnover of the intestinal epithelia in pre-clinical species and human

A.S. Darwich: Lead for literature search, study design, statistical meta-analysis, supervision of U. Aslam, and preparation of manuscript.

U. Aslam: Preliminary literature search on enterocyte turnover in pre-clinical species. The work was carried out as a part of Master of Pharmacy project report.

D.M. Ashcroft: Input on manuscript.

A. Rostami-Hodjegan: Supervision of research, study design, input on data analysis and manuscript preparation.

Chapter 6:

In preparation

Development and assessment of a nested enzyme-within-enterocyte turnover model for mechanism-based inhibition in the small intestine

A.S. Darwich: Lead for study design, literature search, PBPK modelling development and simulation and preparation of manuscript.

D.M. Ashcroft: Input on manuscript.

A. Rostami-Hodjegan: Supervision of research, input on PBPK modelling development and simulation, input on manuscript.

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**Chapter 2: Trends in oral drug
bioavailability following bariatric
surgery: examining the variable
extent of impact on exposure of
different drug classes**

Chapter 2: Trends in oral drug bioavailability following bariatric surgery: examining the variable extent of impact on exposure of different drug classes

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2.1 Abstract

2.1.1 Aims

To identify the most commonly prescribed drugs in a bariatric surgery population and to assess existing evidence regarding trends in oral drug bioavailability post bariatric surgery.

2.1.2 Methods

A retrospective audit was undertaken to document commonly prescribed drugs amongst patients undergoing bariatric surgery in an NHS hospital in the UK and to assess practice for drug administration following bariatric surgery. The available literature was examined for trends relating to drug permeability and solubility with regards to the Biopharmaceutics Classification System (BCS) and main route of elimination.

2.1.3 Results

No significant difference in the ‘post/pre surgery oral drug exposure ratio’ (ppR) was apparent between BCS class I to IV drugs, with regards to dose number (Do) or main route of elimination. Drugs classified as ‘solubility limited’ displayed an overall reduction as compared with ‘freely soluble’ compounds, as well as an unaltered and increased ppR.

2.1.4 Conclusion

Clinical studies establishing guidelines for commonly prescribed drugs, and the monitoring of drugs exhibiting a narrow therapeutic window or without a readily

assessed clinical endpoint, are warranted. Using mechanistically based pharmacokinetic modelling for simulating the multivariate nature of changes in drug exposure may serve as a useful tool in the further understanding of postoperative trends in oral drug exposure and in developing practical clinical guidance.

2.2 Summary

2.2.1 What is already known about this subject

Changes to oral drug bioavailability have been observed post bariatric surgery. However, the magnitude and the direction of changes have not been assessed systematically to provide insights into the parameters governing the observed trends. Understanding these can help with dose adjustments.

2.2.2 What this study adds

Analysis of drug characteristics based on a biopharmaceutical classification system is not adequate to explain observed trends in altered oral drug bioavailability following bariatric surgery, although the findings suggest solubility to play an important role.

2.3 Introduction

Obesity is generally defined by the body mass index ($\text{BMI} = \text{Body Weight (kg)} / \text{Height (m)}^2$). The classification is somewhat arbitrary such that ‘overweight’ means a $\text{BMI} \geq 25$ but $<30 \text{ kg}\cdot\text{m}^{-2}$, ‘obesity’ refers to $\text{BMI} \geq 30$ but $<40 \text{ kg}\cdot\text{m}^{-2}$ and ‘morbid obesity’ is a $\text{BMI} \geq 40 \text{ kg}\cdot\text{m}^{-2}$ (this may also refer to being obese and suffering from related co-morbid conditions) (WHO, 2006; Picot *et al.*, 2009).

Over the last decade the prevalence of obesity has increased dramatically in the USA and Europe. In the USA 32.2% of the male and 35.5% of the female population over the age of 20 years were characterised as obese in 2007-2008 (Flegal *et al.*, 2010). The United Kingdom has the highest reported obesity rate in Europe (OECD, 2011). In England, 24.1% of the male and 24.9% of the female population over the age of 16 years were classified as obese in 2008 (OHE, 2010). Bariatric surgery has proven to be successful in treating morbid obesity. In the USA and Canada approximately 200,000

bariatric surgeries were performed in 2008 (Buchwald and Oien, 2009). In England 4,221 surgeries were performed in 2008/09, an increase of over 100% since 2006/07 (Picot *et al.*, 2009; The NHS Information Centre, 2010). Several bariatric surgical methods currently coexist in healthcare. These include the adjustable gastric band (AGBD), sleeve gastrectomy (SG), biliopancreatic diversion (BPD), biliopancreatic diversion with duodenal switch (BPD-DS) and Roux-en-Y gastric bypass (RYGB) (National Institutes of Health, 2010). Other procedures, such as jejunoileal bypass (JIB), have been gradually phased out due to a higher likelihood of adverse events (Griffen *et al.*, 1977; Elder and Wolfe, 2007; Singh *et al.*, 2009).

Bariatric surgical procedures have been well described in the literature (Schneider and Mun, 2005; Elder and Wolfe, 2007), where they are generally characterised as being restrictive, in terms of physiologically reducing dietary intake, malabsorptive, through reducing the ability of the gastrointestinal (GI) tract to absorb nutrients or a combination of both. Restrictive procedures such as AGBD and SG result in a reduced gastric capacity to 15-20 mL and 60-80 mL respectively (Schneider and Mun, 2005; Lee *et al.*, 2007). The JIB, considered a malabsorptive procedure, results in a 90-95% bypass of the small intestine, retaining the duodenum, proximal jejunum and terminal ileum (Griffen *et al.*, 1977; Elder and Wolfe, 2007; Singh *et al.*, 2009). The BPD-DS, primarily a malabsorptive procedure, results in a reduced gastric volume (100-175 mL) and bypass of larger parts of the small intestine, forming a biliopancreatic canal transporting the bile juices to the distal ileum (Hess and Hess, 1998; Spak *et al.*, 2010). The RYGB, combining restriction and malabsorption, results in the restriction of the stomach to 15-30 mL, and bypass of the proximal small intestine (Wittgrove and Clark, 2000; DeMaria *et al.*, 2002; Spak *et al.*, 2010).

Bariatric surgery imposes a number of physiological alterations known to affect the bioavailability of orally administered drugs (F_{oral}), dependent on the fraction of drug that is absorbed in the intestinal gut wall (f_a), the fraction that escapes gut wall metabolism (F_G), and the fraction that escapes hepatic metabolism (F_H) (Equation 1.1).

$$F_{oral} = f_a \cdot F_G \cdot F_H$$

Equation 1.1: Components of F_{oral} .

f_a and F_G are highly influenced by drug specific properties, such as permeability and solubility, and the GI physiology such as gastric emptying time, GI pH profiles, small intestinal transit time, GI drug metabolising enzymes and GI efflux transporters (Rowland and Tozer, 1989; Jamei *et al.*, 2009). Gastric emptying time can serve as the rate limiting step for highly permeable and highly soluble drugs as the absorption from the stomach is low (Higaki *et al.*, 2008). The gastrointestinal pH may affect drug dissolution of permeability-limited drugs displaying a pK_a within the range of the GI pH fluctuations. Small intestinal transit time can influence the drug absorption of poorly soluble or extended release drug formulations (Rowland and Tozer, 1989).

Metabolism in the gut acts to regulate oral bioavailability of drugs and other xenobiotics, and is an important determinant in the metabolism of substrate drugs (Kolars *et al.*, 1994). CYP3A4 is the most abundant drug metabolising enzyme in the GI tract, preceding CYP2C9/19 amongst others in order of appearance (Peters *et al.*, 1989; Fisher *et al.*, 2001; Paine *et al.*, 2006; Riches *et al.*, 2009). CYP3A4 and CYP3A5 are both present along the GI tract, where CYP3A4 expression rises towards the jejunum to decrease towards the ileum (Kolars *et al.*, 1994; Paine *et al.*, 1997). GI transporters may influence the absorption of orally administered drugs and potentially also the extent of metabolism in the gut through active substrate efflux (Benet and Cummins, 2001). Numerous transporters are present in the gut, where P-glycoprotein (P-gp) is perhaps the most extensively studied of the GI transporters. The relative expression pattern of P-gp in the small intestine increases from the proximal to the distal parts of the small intestine (Mouly and Paine, 2003).

The Biopharmaceutics Classification System (BCS) classifies drugs in accordance to solubility and permeability. Solubility takes on the form of a dose number (Do), given by dividing highest dose strength in mg (M_0) by a volume of 250 mL (V_0) divided by the aqueous solubility of the drug ($\text{mg} \cdot \text{mL}^{-1}$) over a pH range of 1.0-7.5 at 37°C (C_s) (FDA, 2000). Defining $Do \leq 1$ as highly soluble and an $f_a \geq 90\%$ as a highly permeable drug, drugs are classified as class I (high solubility-high permeability), class II (poor solubility-high permeability), class III (high solubility-poor permeability) and class IV (poor solubility-poor permeability) (Amidon *et al.*, 1995).

The aims of this study were to identify the most commonly prescribed drugs in a bariatric surgery population and to assess existing evidence with respect to altered oral drug bioavailability post bariatric surgery. This would be carried out through methodologically reviewing the current literature, evaluating drug specific pharmacokinetic characteristics relating to solubility, permeability and main route of elimination.

2.4 Methods

2.4.1 Evaluation of drug utilisation following gastric bypass

A retrospective audit of drug utilisation by bariatric surgery patients was performed at Salford Royal NHS Foundation Trust, Salford, UK. Data collection was performed using the hospitals electronic patient record (EPR) system, iSOFT clinical manager 1.4, which incorporates the medication prescription and administration records. A search of the EPR system was carried out for all patients under the care of a consultant bariatric surgeon. The search consisted of patients that had undergone surgery in the previous 5 months, from the 21st March 2011. The medical history of patients was initially searched to identify those having undergone laparoscopic RYGB. Patients who had a colostomy, gastric banding and reversal of gastric banding were excluded.

Data extraction was performed utilising an anonymous data collection form, maintaining patient confidentiality. Information extracted consisted of type of bariatric surgical procedure, pre surgery prescribed drug therapy and associated co-morbidities, post surgery medication including formulation changes and documented reasons behind alterations. Pre surgery medications were compared to the patients' medical charts on discharge, generally 2-3 days post-surgery. Statistical analysis of trends in prescribed drugs observed during the retrospective audit was conducted using McNemar's non-parametric test ($P \leq 0.05$) in R v 2.12 (the R Foundation for Statistical Computing).

2.4.2 Review and analysis of oral drug bioavailability following gastric bypass

Embase (1980-2010) and PubMed (1977-2010) were searched using the following combinations of key words: 'oral administration or bioavailability', 'absorption',

'bioavailability', 'gastric bypass', 'jejunoileal bypass', 'bariatric surgery'. In addition, references of related articles were systematically investigated for relevant publications.

Initial screening of titles and abstracts was carried out to identify those compliant with pre specified criteria of reporting observational trends in bioavailability/oral drug exposure of pharmaceutical agents following bariatric surgery or the identification of adverse events related to oral drug exposure following surgery. Studies excluded consisted of gastric surgical procedures not related to obesity, reports on nutrients or supplementation post bariatric surgery, publications written in a language other than English. Screening was carried out to determine inclusion or exclusion criteria.

Information extracted included study characteristics: surgical procedure, study design, number of participants, year of publication, country of origin and time since procedure; study population characteristics: sex, average age, average BMI and co-morbidities. The principle measurement of bioavailability in the analysis was area under the curve (AUC), bioavailability, steady-state plasma or serum concentration.

Observed trends in oral drug exposure were assumed to follow a log normal distribution. Quantitative analysis was carried out through estimating the mean effect size of response ratios and their variance following random-effect model. Statistical analysis was carried out with a two-tailed t-test of the standard normal cumulative distribution (Borenstein *et al.*, 2009). Statistical analysis between subgroups were carried out utilising Welch's t-test ($P \leq 0.05$) of log-transformed weighted means and SDs with *post hoc* Dunn-Šidák correction ($P \leq 0.05$) using Microsoft® Excel 2003 and Matlab 2010 (the Mathworks Inc).

2.5 Results

2.5.1 Evaluation of clinical drug utilisation following gastric bypass

The search of iSOFT identified 63 patients under the care of the bariatric surgeon and 38 patients (26 female) with a mean age of 45 (range 23-64) years were eligible for data extraction after fulfilling the pre-specified criteria. The surgical procedures performed included laparoscopic RYGB (n=34), laparoscopic RYGB with abdominal wall hernia repair (n=3) and conversion of AGBD to RYGB (n=1). Commonly treated

comorbidities amongst the study population included hypertension (n=12), type 2 diabetes (n=15), depression/anxiety (n=11), hypothyroidism (n=5), osteoarthritis (n=11), hypercholesterolemia (n=10) and asthma (n=9).

The most commonly prescribed drugs prior to surgery included statins (n=13), ACE inhibitors (n=10), proton pump inhibitors (PPIs)/H₂-receptor antagonists (n=10) and metformin (n=10). Comparing pre to post surgery, a significant increase in the prescription of paracetamol, opioids, PPIs/H₂ receptor antagonists, heparin and antimicrobials was observed ($P<0.05$) as well as an overall reduction in the number of patients treated for type 2 diabetes ($P<0.05$). The most common drugs prescribed following surgery included heparin (n=38), PPIs/H₂ receptor antagonists (n=38) and paracetamol (n=34). The number of patients prescribed cardiovascular agents remained constant postoperatively, whereas prescriptions of statins displayed a non-significant reduction of 31% ($P>0.05$). The postoperative formulation of choice for diuretics was liquid (n=4), whereas the remaining cardiovascular agents were tablets that were being crushed postoperatively (n=28) (Figure 2.1).

All patients receiving antidepressants remained on the same antidepressant post surgery, with all but one receiving a different formulation. Of the 11 patients pre-scribed antidepressants, 50% were switched on to liquid formulations, whereas the remaining 50% were advised to crush their tablets post surgery (Figure 2.1). All patients with a prior diagnosis of diabetes underwent a diabetic review during their stay in hospital. The review resulted in a significant reduction in post-surgical prescriptions of anti-diabetic medications by 67% ($P<0.05$). Patients who no longer required diabetic medication were alternatively switched to manual monitoring of blood glucose concentrations. Metformin was the only agent continued postoperatively and in 60% of cases continued at a reduced dose of up to a third of the pre-surgical dose level. All but one patient were converted to liquid preparations (Figure 2.1). Standard postoperative treatment consisted of 1-2 weeks low molecular weight heparin injection, PPIs (lansoprazole FasTab) and liquid formulation pain-killers (codeine and paracetamol) being prescribed for all patients. This patient group also displayed a significant increase in the prescription of PPIs/H₂ receptor antagonists, opioids, paracetamol and heparin ($P<0.05$). One patient with a history of deep vein thrombosis remained on tinzaparin for 4 weeks.

Lansoprazole was given at a dose of 30 mg twice daily as a orodispersible formulation. The prophylactic therapy was to continue for at least 6 months postoperatively, before reducing the dose to once daily for a further 18 months. Approximately 2 weeks after surgery the sublingual formulation was switched to the solid tablet or capsule formulation.

Antimicrobials were given to 7 patients post-operatively for the eradication of *Helicobacter pylori* (n=5) that was detected from an intra-operative gastric mucosal biopsy, development of hospital-acquired pneumonia (n=1) and anastomotic leakage (n=1). All patients were given liquid preparations.

In total 17 patients were taking analgesics on regular basis prior to surgery, increasing to 38 patients postoperatively. Analgesic products included paracetamol (n=2, $P<0.05$), aspirin (n=5), opioids (n=9, $P<0.05$) and non-steroidal anti-inflammatory drugs (NSAIDs) (n=3). Patients taking NSAIDs prior to surgery (n=3) were advised to stop taking these postoperatively due to an increased risk of developing gastro-jejunal anastomotic ulceration.

As stated in the patients 'plan' for postoperative care, a review of the nutritional progress usually occurred approximately 2 weeks post surgery. Patients were therefore advised to cease taking any non-essential vitamins and minerals immediately after surgery until the nutritional review had been completed. On discharge patients were informed that they would require taking lifelong dietary supplementation.

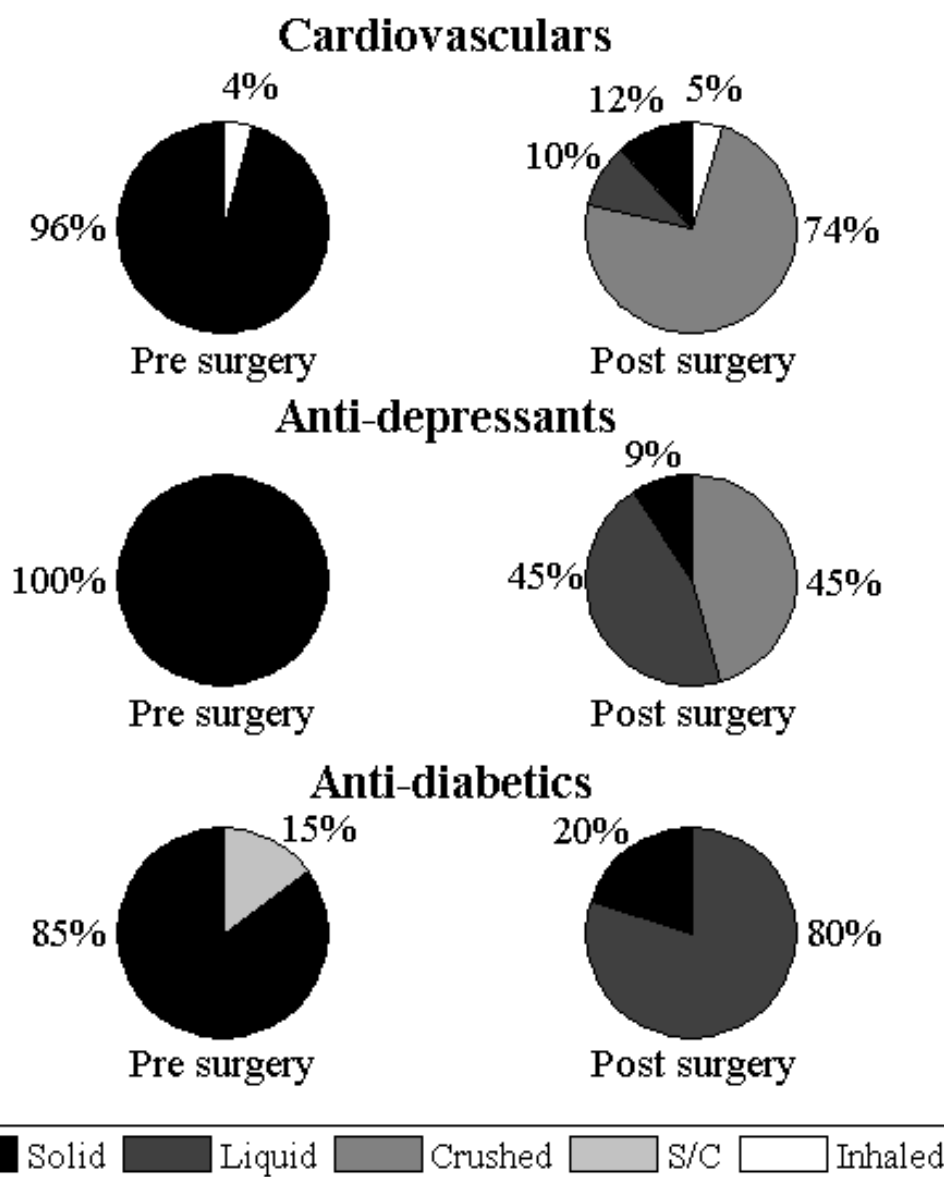


Figure 2.1. Pharmacotherapeutic alterations in formulation properties post bariatric surgery (Solid=solid tablets, Liquid=liquid formulation, S/C=subcutaneous, Crushed=patients instructed to crush tablets, Inhaled=inhalation formulation) of prescribed cardiovascular drugs, anti-depressants and anti-diabetics as compared to prior to surgery observed in 38 evaluated patients.

2.5.2 Oral drug bioavailability following bariatric surgery

The initial search of Embase and PubMed identified 311 potentially relevant publications based on search terms. After screening of abstracts, 66 articles were identified of which 22 matched the pre-specified criteria following full text screening.

Overall, the literature search included 41 articles (20 controlled trials, 18 case reports and three case series) published between 1974 and 2011 that were suitable for further evaluation and data extraction.

Articles relating to JIB mainly appeared between 1974 and 1985. An increase of published data on RYGB was identified between 2000 and 2011, following the trend of RYGB being the most widely used bariatric surgical procedure at the present time (Picot *et al.*, 2009).

Surgical techniques identified included RYGB (n=14), JIB (n=19), reversal of jejunioileal bypass (JIB R) (n=4), BPD-DS (n=2) BPD (n=3), GBP (n=1) and AGBD (n=1) (Table 2.1). The 41 identified publications originated from the USA (58%), followed by the UK (10%), Italy (5%), Norway (5%) and Canada (5%).

A total of 230 participants were studied in the identified publications. The time point for post surgical examination of oral drug exposure ranged from 0.1 to 88.9 months (Fuller *et al.*, 1986; Rogers *et al.*, 2008). In total 38 drugs were identified. These were categorically divided based on therapeutic indication. The studied drugs consisted of antimicrobials (n=12 drugs), cardiovascular drugs (n=2), immunosuppressants (n=4), antiepileptics (n=3), analgesics (n=2), oral contraceptives (n=4), anti-ulcer drugs (n=1), statins (n=1), thyroid hormones (n=1), anti-depressants (n=2), anti-cancer drugs (n=2), anti-diabetics (n=1) and HIV medication (n=1). Postoperative trends in drug bioavailability based on geometric mean drug exposure ranged from a 10.43 fold increase with a 95% confidence interval (CI) ranging from 0.10 to 1058 (n=32) (Terry *et al.*, 1982) to a 5.88 fold reduction (n=1) (Liu and Artz; Marcus *et al.*, 1977; Gerson *et al.*, 1980; Adami *et al.*, 1991; Cossu *et al.*, 1999; Skottheim *et al.*, 2009; Skottheim *et al.*). The overall post/pre surgical oral drug exposure ratio ('ppR') obtained from meta-analysis significantly diverged from pre-surgery with a mean ppR of 0.80 with a 95% confidence interval (CI) of 0.67 to 0.94 ($P<0.01$), when analysing quantitative data providing mean and variance of exposure pre and post bariatric surgery.

Table 2.1. Controlled trials examining the trend in oral drug exposure following bariatric surgery.

	Drug	Surgery	Pre to post surgery oral drug exposure ratio (X, 95% CI)	Patients (n)	References
▲	Phenoxymethyl penicillin 1,000 mg	JIB	10.43 (0.10, 1058)*	3	(Terry <i>et al.</i> , 1982)
	Atorvastatin acid 20-80 mg	BPD-DS	1.85 (0.81, 4.27)†	10	(Skottheim <i>et al.</i> , 2010)
—	Ranitidine 300 mg	BPD	1.43 (1.12, 1.81)*	11	(Cossu <i>et al.</i> , 1999)
	Metformin 1,000 mg	RYGB	1.20 (0.91, 1.58)†	16	(Padwal <i>et al.</i>)
	Propylthiouracil 400 mg	JIB	1.09 (0.84, 1.42)†	6	(Kampmann <i>et al.</i> , 1984)
	Phenazone 15 mg/kg	JIB	1.06 (0.81, 1.38)‡	17	(Andreasen <i>et al.</i> , 1977)
	Atorvastatin acid 20-80 mg	RYGB	1.00 (0.29, 3.46)†	12	(Skottheim <i>et al.</i> , 2009)
	Paracetamol 1,500 mg	JIB	1.00 (0.647, 1.54)*	3	(Terry <i>et al.</i> , 1982)
	Digoxin 0.5 mg daily (First day: 1 mg)	JIB	0.89 (0.70, 1.14)†	7	(Marcus <i>et al.</i> , 1977)
	Erythromycin 250 mg	GBP	0.61 (0.38, 0.99)†	7	(Prince <i>et al.</i> , 1984)
	Sulfisoxazole 1,000 mg	JIB	0.84 (0.74, 0.94)*	3	(Garrett <i>et al.</i> , 1981)
	Norethisterone 3 mg	JIB	0.80 (0.39, 1.63)‡	6	(Victor <i>et al.</i> , 1987)
▼	Digoxin 0.5 mg	JIB	0.76 (0.59, 0.97)†	9	(Gerson <i>et al.</i> , 1980)
	MMF 2·1,000 mg	RYGB	0.66 (0.21, 2.06)*	2	(Rogers <i>et al.</i> , 2008; Genentech, 2010)
	Levonorgestrel 0.25 mg	JIB	0.55 (0.34, 0.90) ‡	6	(Victor <i>et al.</i> , 1987)
	Sirolimus 8 mg	RYGB	0.54 (0.25, 1.17)*	4	(Brattstrom <i>et al.</i> , 2000; Mathew <i>et al.</i> , 2006; Rogers <i>et al.</i> , 2008)
	Hydrochlorothiazide 75 mg	JIB	0.46 (0.33, 0.65)*	4	(Beermann and Groschinsky-Grind, 1977; Backman <i>et al.</i> , 1979)
	Sertraline 100 mg	RYGB	0.40 (0.19, 0.84)†	5	(Roerig <i>et al.</i>)
	Ampicillin (pivampicillin 750 mg)	JIB	0.37 (0.16, 0.89)†	5	(Kampmann <i>et al.</i> , 1984)
	Phenytoin 200 mg	JIB	0.32 (0.17, 0.58)†	7	(Kennedy and Wade, 1979)

▲ = Indicating a significant increase in oral drug exposure (AUC, F_{oral} or steady state concentration) following surgery. — = No statistical significant change in oral drug exposure. ▼ = Significant reduction in oral drug exposure. X=mean ratio change based on geometric mean, CI=95% confidence interval. GBP=Gastric Bypass (gastroplasty and Roux-en-Y gastric bypass), JIB=Jejunioileal Bypass, BPD=Biliopancreatic Diversion, BPDDS=Biliopancreatic Diversion with a Duodenal Switch, RYGB=Roux-en-Y Gastric Bypass, MMF=mycophenolate mofetil. *t-test performed at 5% significance level. †Statistical outcome as reported in publication. ‡Welch's t-test at a 5% significance level.

2.5.3 Analysis in accordance to the biopharmaceutics classification system

Classifying drugs into BCS classification, class I (high solubility, high permeability), class II (low solubility, high permeability), class III (high solubility, low permeability) and class IV (low solubility, low permeability), identified eight drugs as BCS class I (n=66 patients), three drugs as BCS class II (n=7), eleven drugs as BCS class III (n=53) and three drugs as BCS class IV (n=8). A total of eight drugs were found to be inconclusive (n=40). Information was lacking in the literature with regards to the BCS classification of pivampicillin, para-aminosalicylic acid and lopinavir/ritonavir.

Of the eight drugs identified as BCS class I, four drugs displayed a reduction in exposure following surgery, four drugs remained unaltered and one drug displayed an increase in drug exposure. Out of eleven mapped BCS class III drugs, five displayed a reduction in drug exposure following surgery. An additional five drugs displayed unaltered drug exposure, whereas one drug displayed an increase. All BCS class II and IV drugs (total of six) displayed a reduction in drug exposure following surgery (Figure 2.2).

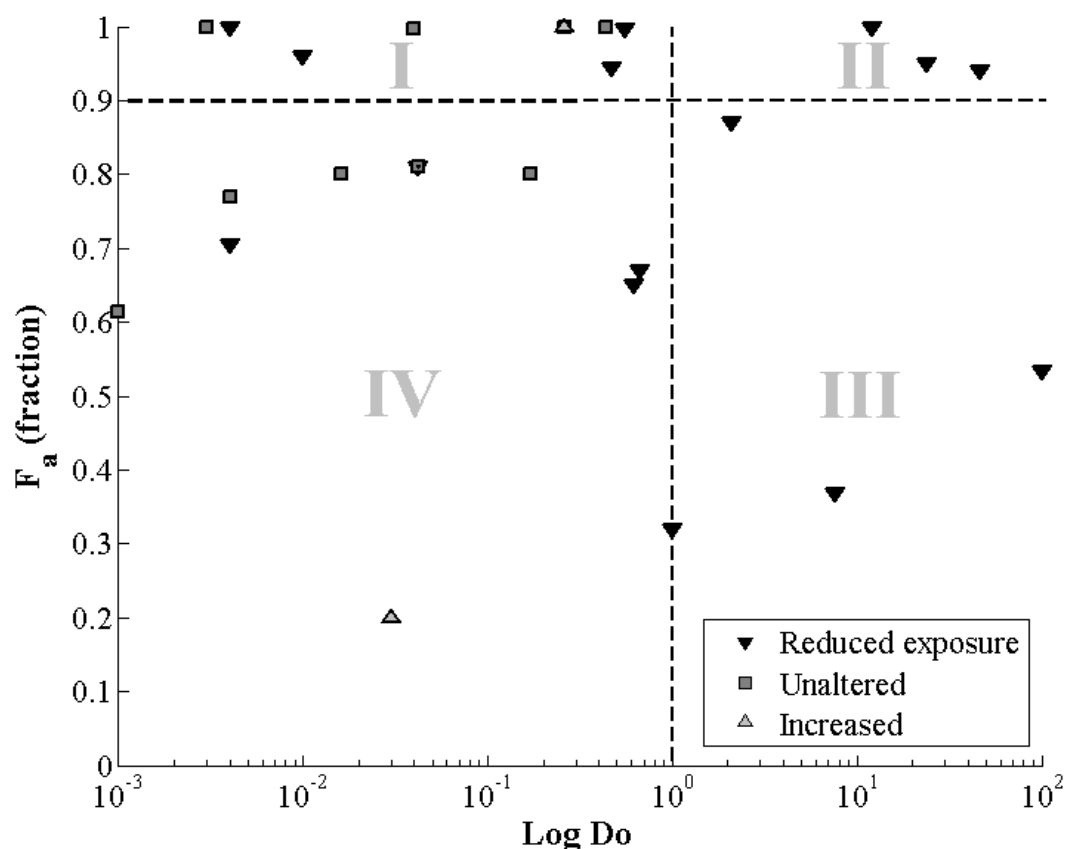


Figure 2.2. Categorical trends in oral drug exposure in relation to f_a (fraction of orally administered dose absorbed) and Do (dose number) in accordance to the BCS dividing drugs into BCS class I-IV). Reduced exposure (\blacktriangledown); Unaltered (\square); Increased (\triangle) (Kaplan *et al.*, 1972; Kampmann and Skovsted, 1974; Patel *et al.*, 1975; Wenzel and Kirschsieper, 1977; Nelson *et al.*, 1982; Oie *et al.*, 1982; Dressman *et al.*, 1985; Kearney *et al.*, 1993; Stewart *et al.*, 1995; Crowe and Lemaire, 1998; Peloquin *et al.*, 1999; Tavelin *et al.*, 1999; Lennernas *et al.*, 2002; Tamura *et al.*, 2002; Bock *et al.*, 2003; Garekani *et al.*, 2003; Lennernas, 2003; Yalkowsky and He, 2003; Bolton *et al.*, 2004; Kasim *et al.*, 2004; Lindenberg *et al.*, 2004; Wu and Benet, 2005; Song *et al.*, 2006; Ashiru *et al.*, 2008; Becker *et al.*, 2008; Ni *et al.*, 2008; Petan *et al.*, 2008; Chemical, 2010; FDA, 2010; BNF, 2011; NCBI, 2011).

Analysing BCS classified drugs where studies provided quantifiable measurements of drug exposure (*i.e.* AUC, F_{oral} and plasma or serum concentration levels), combining weighted means and variance of pre/post drug exposure ratio, BCS class I ($n=5$ drugs, $n=108$ population) displayed a weighted mean ppR of 0.94 (CI 0.66, 1.34). BCS class II

(n=2 drugs, n=5 population) displayed a weighted mean ppR of 0.80 (CI 0.48, 1.36), BCS class III (n=8 drugs, n=111 population) showed a weighted mean ppR of 0.86 (CI 0.68, 1.10), whereas BCS class IV (n=2 drugs, n=17 population) displayed a weighted mean ppR of 0.51 (CI 0.22, 1.17). Statistical analysis did not reveal any significant differences from pre-surgical ratio of 1 between BCS subgroups ($P>0.05$) (Figure 2.3).

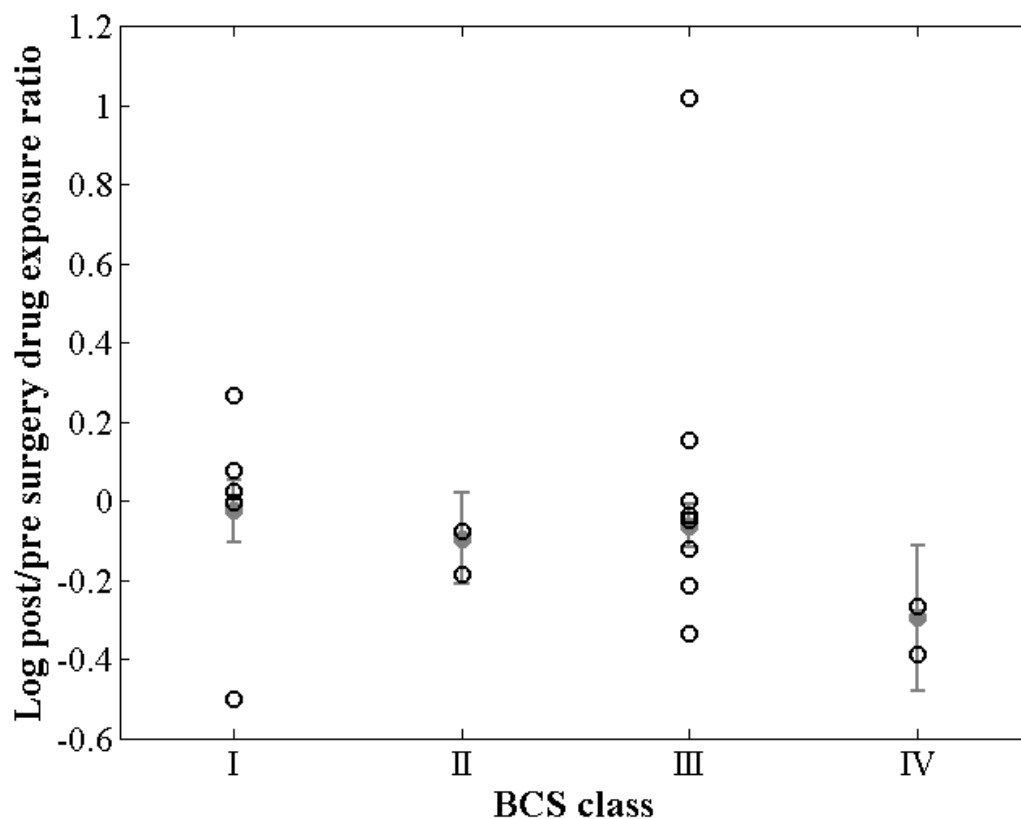


Figure 2.3. Log mean post/pre surgery drug exposure ratio of BCS class I-IV drugs. ○ log mean drug ratio, ● combined log mean ratio and standard deviation of subgroup.

Drugs where studies provided quantifiable measurements of drug exposure were further statistically analysed with regards to $Do \leq 1$, BCS class I and III (n=16 drugs, n=262 population) vs. BCS class II and IV (n=4 drugs, n=48 patients). $Do \leq 1$ drugs displayed a weighted mean ppR of 0.83 (0.69-1.00), whereas $Do > 1$ drugs displayed a ratio of 0.70 (95% CI 0.45, 1.10). Statistical analysis revealed no statistical significance from a pre surgical ratio of 1 or between subgroups ($P>0.05$) (Figure 2.4).

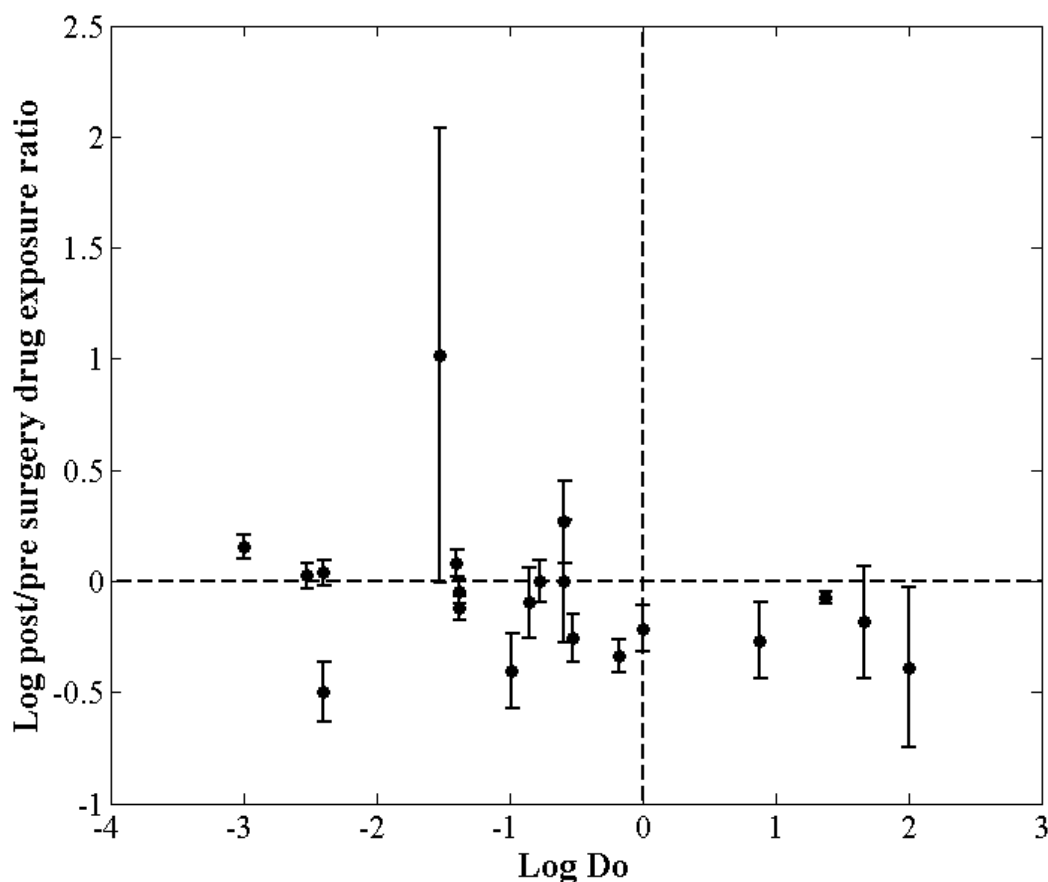


Figure 2.4. Mean post/pre surgery drug exposure ratio and standard deviation in relation to quantitative Do (dose number).

2.5.4 Analysis in accordance to main route of elimination

Examining drugs in accordance to the main route of elimination produced a weighted mean ppR in oral drug exposure of 0.83 (95% CI 0.59, 1.17) for CYP3A4/5 substrates (n=7 drugs, n=99 patients), 0.32 (95% CI 0.14, 0.72) for CYP2C substrates (n=1 drug, n=16 population), 0.90 (95% CI 0.68, 1.18) for mainly renally-cleared drugs (n=5 drugs, n=103 population) and 0.76 (95% CI 0.57, 1.01) for the remaining drugs (n=8 drugs, n=92 population). Statistical analysis revealed no difference in ppR between the subgroups ($P>0.05$), whereas the CYP2C subgroup significantly differed from the pre-surgical ratio of 1 ($P<0.001$).

2.6 Discussion

2.6.1 *Evaluation of drug utilisation following gastric bypass*

The observed practice of altering formulation properties to liquid preparations are considered necessary in healthcare due to the postoperative condition of the patient rather than as a proactive measure against altered pharmacokinetics due to changes in GI physiology. Patients are advised to remain on liquid formulations for approximately 2-3 weeks, varying nationally to 3 months to lifelong, post bariatric surgery to prevent any unnecessary strain on the gastric and jejunal transection lines and the gastrojejunal anastomosis and therefore to allow time for healing. As an unintentional consequence changing to liquid preparations may result in an increase in oral bioavailability for solubility limited drugs.

Pharmacotherapeutic treatment of type 2 diabetes was ceased in 67% of patients following surgery. The prescription of metformin remained unaltered following surgery, albeit being observed to be significantly reduced 12 months postoperatively, by Malone and Alger-Mayer, following 114 patients up to 24 months post surgery (Malone and Alger-Mayer, 2005).

Antidepressants, TCAs and SSRIs were continued immediately postoperatively in all cases. This was consistent with the report by Malone and Alger-Mayer, indicating prescriptions of TCAs and SSRIs remained statistically unaltered 12 months post surgery.

Vitamin and mineral deficiencies are likely to occur indefinitely in the bariatric patient, resulting in the need for lifelong supplementation (Ponsky *et al.*, 2005). Deficiencies are most likely to occur with fat-soluble vitamins (A, D, E and K), calcium and iron. Calcium and iron absorption is highly influenced by the reduction of hydrochloric acid production within the stomach after bariatric surgery (Ponsky *et al.*, 2005).

Medication reviews have been performed observing modifications to patient dosing and formulation after bariatric surgery. Currently no consensus guidelines are available regarding considerations of pharmacotherapy post bariatric surgery. Evidence based

national guidelines are warranted as bariatric surgery is becoming a more popular method for the treatment of obesity (Buchwald and Williams, 2004).

2.6.2 Oral drug exposure following bariatric surgery

Reviewing current data on changes in drug exposure prior to, and post bariatric surgery reveals many uncertainties regarding the prediction of post bariatric surgery drug bioavailability and the mechanisms behind these changes. BCS did not prove to be enough to explain the observed trend.

Post-bariatric surgery imposed restrictions on gastric volume (*e.g.* SG and RYGB) has been observed to reduce the gastric emptying time of liquids (Horowitz *et al.*, 1982; Braghetto *et al.*, 2009) and may further lead to an increase in gastric pH (Smith *et al.*, 1993; Behrns *et al.*, 1994). This together with a reduced fluid intake may impact the solubility of orally administered drugs.

Statistical analysis did not present any significant trends when examining BCS class I-IV, Do or elimination subgroups. None of the Do>1 classified drugs displayed an increase in bioavailability postoperatively, whereas the Do≤1 group exhibited a larger variability in post/pre surgery drug exposure outcome. This may be due to solubility issues of the Do>1 group, resulting in an overall reduction in oral drug exposure following surgery. The impact is however unclear due to a low number of drugs falling into the Do>1 category, where further clinical data is necessary to establish the case. Due to the restriction of the gastric volume following certain types of bariatric surgery (*e.g.* RYGB and BPD-DS) the default concomitant fluid intake of 250 mL in the BCS may no longer be valid. This will have implications for shifting the boundaries between BCS class I/III and II/IV, such that some freely soluble drugs may become solubility limited dependent on the administered dose. This is further complicated by a potentially altered gastric pH (Smith *et al.*, 1993; Behrns *et al.*, 1994; FDA, 2000; Schneider and Mun, 2005; Elder and Wolfe, 2007).

A small intestinal bypass will reduce the absorption area and may also alter the regional distribution and abundances of drug metabolising enzymes and transporters thus altering exposure of substrate drugs. When examining drugs with respect to main route

of elimination, no significant difference was observed between CYP3A, CYP2C, renal and other drugs. These results were also associated with a high degree of uncertainty due to scarcity of data, albeit a higher ppR of CYP3A may be expected due to the GI abundance of CYP enzymes where CYP3A4 is the most highly abundant. The bypass of highly abundant regions of CYP3A4 may lead to an increase in oral bioavailability while such an effect may become less relevant for substrates due to decreasingly abundant CYP2C9/19 and CYP2D6. Such a hypothesis may be supported by the observed trend in AUC of atorvastatin acid, mainly metabolised by CYP3A4 (Lennernas and Fager, 1997), thus potentially displaying an increase in bioavailability post malabsorptive bariatric surgery due to the bypass of significant segments GI regions highly abundant of CYP3A4 (Paine *et al.*, 1997), whereas this effect may be counteracted by a reduced absorption area. Following BPD-DS a significant increase in AUC of atorvastatin acid (2-fold) was observed, whereas no significant change was observed following RYGB, thus potentially increasing the risk of adverse effects, such as myopathy, following BPD-DS (Omar *et al.*, 2001; Skottheim *et al.*, 2009; Skottheim *et al.*, 2010).

The lack of quantifiable drug exposure data means that drugs displaying a low F_G or limited absorption prior to surgery are likely to be wrongly classified when trying to generalise over a wide variety of drugs, such as metformin and phenoxymethylpenicillin.

Metformin, a highly soluble and permeability limited basic compound (van de Merbel *et al.*, 1998; Kasim *et al.*, 2004) has been suggested to be subject to saturable transporter uptake to an extent by organic cation transporters in the intestine although not fully understood, thus resulting in a dose-dependent absorption that is mainly renally-cleared (Tucker *et al.*, 1981; Proctor *et al.*, 2008). The observed increase in postoperative bioavailability (Padwal *et al.*) might be due to altered small intestinal transit; reductions in gastric emptying time and small intestinal motility would in theory lead to a longer exposure time to enterocytic influx transporters. A further reason could be a post-surgical alteration in transporter distribution patterns. Phenoxymethylpenicillin, considered a highly soluble and permeable compound (Kasim *et al.*, 2004), displayed a significant increase in AUC post-JIB, possibly due to a reduced intestinal degradation by bacterial β -lactamase due to a major small intestinal restriction (Cole *et al.*, 1973).

The different surgical implications on GI physiology may result in variable trends in post-surgery drug exposure across the range of bariatric procedures, as is the case with atorvastatin acid displaying a significant increase in AUC following BPD-DS procedure as compared to no significant change following the less malabsorptive RYGB procedure (Skottheim *et al.*, 2009; Skottheim *et al.*, 2010). Also the case for cyclosporine, implicated to display a reduction in drug exposure following JIB, an exclusively malabsorptive procedure, as compared to remaining unaltered following the restrictive AGBD (Knight *et al.*, 1988; Ablassmaier *et al.*, 2002; Chenhsu *et al.*, 2003).

The outcomes of oral drug exposure of many commonly prescribed drugs in bariatric surgery populations are still unknown, such as many antidepressants and analgesics. Current available clinical data is very valuable. Going forward it is important that further clinical studies are designed taking into the consideration the potential alterations in concentration-time profiles, relating to pharmacokinetic parameters such as t_{max} . Drugs exhibiting narrow therapeutic range or displaying less readily measurable clinical endpoints will require more stringent monitoring after bariatric surgery, such as immunosuppressants and CNS active drugs.

Due to the multiple physiological factors altered in bariatric surgery (*i.e.* gastric volume, absorption area, CYP-abundance and regional distribution), and the fact that various drugs might be affected to different degrees by each of these changes, physiologically-based pharmacokinetic (PBPK) modelling may help in elucidating the impact of various bariatric surgeries on different drugs given at different doses (Schneider and Mun, 2005; Elder and Wolfe, 2007). Such investigation was outside the scope of the current research however initial attempts on this approach are addressed in another report (Darwich *et al.*, 2012) where the complex nature of interplays were manifested.

In conclusion, based on current findings, analysis of general pharmacokinetic parameters alone (*i.e.* solubility, permeability and main route of elimination) is not enough to explain observed trends in oral drug bioavailability following bariatric surgery, although the findings of this study suggest solubility to potentially play an important role.

These implications support the hypothesis that there are several physiologic and drug-specific parameters which govern the observed changes in drug exposure, thus calling for a more mechanistic approach, integrating all known parameters.

To the authors' knowledge this is the first publication quantitatively examining oral drug bioavailability in relation to a set of pharmacokinetic, biopharmaceutic and other drug-specific parameters and also in the context of pharmacotherapeutic practice following bariatric surgery. Along with further clinical studies, PBPK modelling may provide essential insights into the significance of individual pharmacokinetic parameters and generate important clinical guidance for a constantly growing post bariatric surgery population. Currently, there seems to be no simple algorithm or decision tree that predicts the variable changes to drug bioavailability following bariatric surgery.

2.7 Acknowledgements

There are no competing interests to declare.

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**Chapter 3: A mechanistic
pharmacokinetic model to assess
modified oral drug bioavailability
post bariatric surgery in
morbidly obese patients:
interplay between CYP3A gut
wall metabolism, permeability
and dissolution**

Chapter 3: A mechanistic pharmacokinetic model to assess modified oral drug bioavailability post bariatric surgery in morbidly obese patients: interplay between CYP3A gut wall metabolism, permeability and dissolution

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3.1 Abstract

3.1.1 Objectives

Due to the multi-factorial physiological implications of bariatric surgery, attempts to explain trends in oral bioavailability following bariatric surgery using singular attributes of drugs or simplified categorisations such as the biopharmaceutics classification system have been unsuccessful.

3.1.2 Methods

Pharmacokinetic post bariatric surgery models were created for Roux-en-Y gastric bypass, biliopancreatic diversion with duodenal switch, sleeve gastrectomy and jejunoileal bypass, through altering the ‘Advanced Dissolution Absorption and Metabolism’ (ADAM) model incorporated into the Simcyp[®] Simulator. Post to pre surgical simulations were carried out for five drugs with varying characteristics regarding their gut wall metabolism, dissolution and permeability (simvastatin, omeprazole, diclofenac, fluconazole and ciprofloxacin).

3.1.3 Key findings

The trends in oral drug bioavailability pre to post surgery were found to be dependent on a combination of drug parameters, including solubility, permeability and gastrointestinal metabolism as well as the surgical procedure carried out.

3.1.4 Conclusions

In the absence of clinical studies, the ability to project the direction and the magnitude of changes in bioavailability of drug therapy, using evidence-based mechanistic pharmacokinetic *in silico* models would be of significant value in guiding prescribers to make the necessary adjustments to dosage regimens for an increasing population of patients who are undergoing bariatric surgery.

3.2 Introduction

The prevalence of obesity has increased dramatically in the USA and Europe over the last decade (Elder and Wolfe, 2007; Flegal *et al.*, 2010; OECD, 2011; Ammori, 2012). Bariatric surgery has proven to be successful in treating morbid obesity. In 2008, approximately 220,000 bariatric surgeries were performed in the USA and Canada, whereas over 66,000 operations were carried out in Europe (Buchwald and Oien, 2009; Picot *et al.*, 2009).

Several bariatric surgical procedures currently coexist in healthcare, being characterised as either restrictive, in terms of reducing gastric capacity, malabsorptive, with regard to restricting the small intestine and/or delaying the bile inlet, or a combination of both (Schneider and Mun, 2005; Lee *et al.*, 2007). These procedures include: adjustable gastric band (AGB), sleeve gastrectomy (SG), biliopancreatic diversion (BPD), biliopancreatic diversion with a duodenal switch (BPD-DS) and Roux-en-Y gastric bypass (RYGB) (National Institutes of Health, 2010). Other procedures have been gradually phased out due to a higher likelihood of adverse events, such as jejunoileal bypass (JIB) (Figure 3.1) (Griffen *et al.*, 1977; Elder and Wolfe, 2007; Singh *et al.*, 2009).

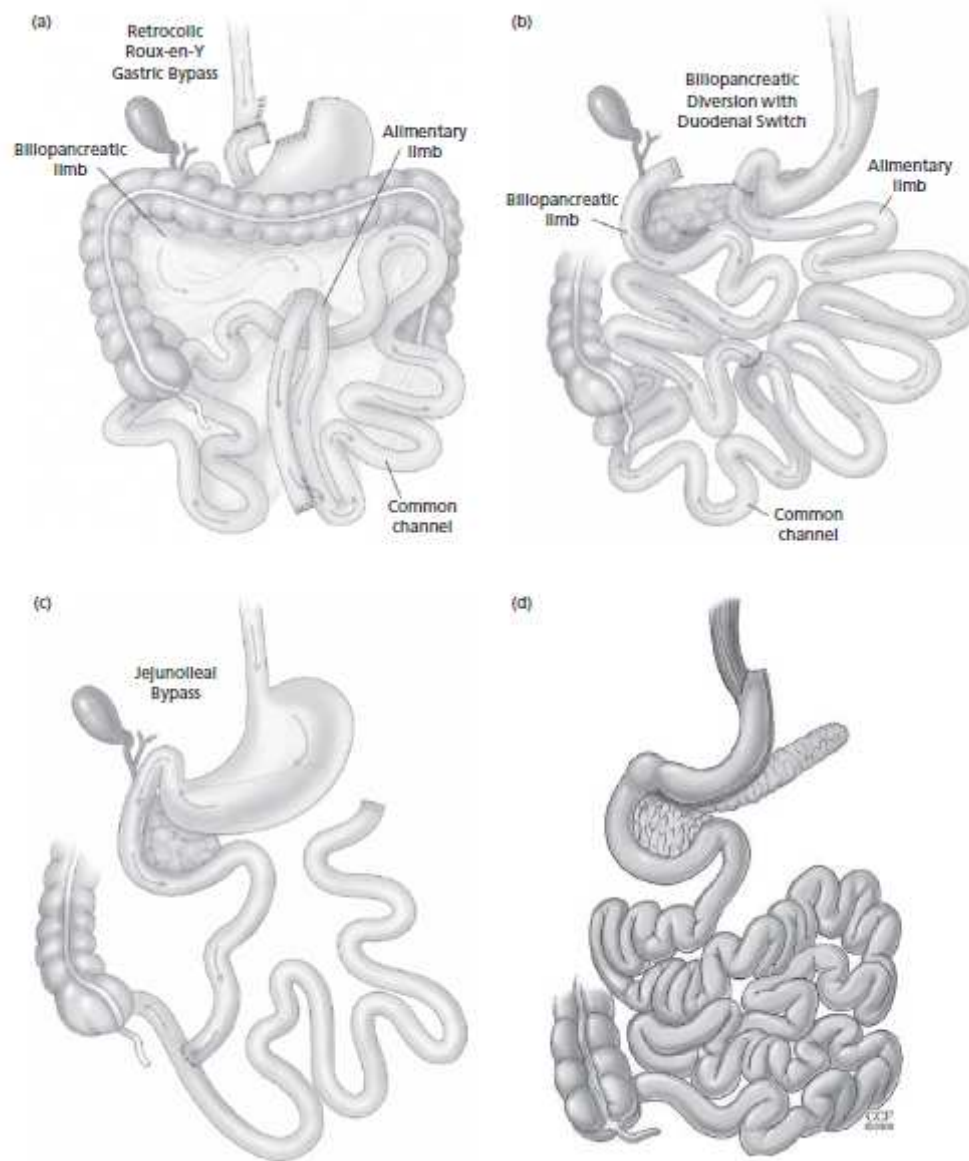


Figure 3.1. Schematic illustrations of a selected bariatric surgical procedures imposing restrictions to the gastrointestinal tract. **A:** Roux-en-Y gastric bypass, **B:** biliopancreatic diversion with duodenal switch, **C:** jejunioileal bypass, obtained from (Elder and Wolfe, 2007), **D:** sleeve gastrectomy, obtained from (Ammori, 2012).

Different types of bariatric surgery will impose a number of physiological changes varying in extent depending on the invasiveness of the procedure. Many of these alterations are known to affect the bioavailability of orally administered drugs, although studies investigating alterations in oral drug exposure pre to post operatively have been limited (Darwich *et al.*, 2012).

Oral bioavailability (F_{oral}) is dependent on the fraction of drug that is absorbed in the intestinal gut wall (f_a), the fraction that escapes gut wall metabolism (F_G), and the fraction that escapes hepatic metabolism (F_H) (Equation 1.1).

$$F_{\text{oral}} = f_a \cdot F_G \cdot F_H$$

Equation 1.1: Components of F_{oral} .

f_a and F_G are highly influenced by drug and formulation properties, such as disintegration, dissolution, permeability, solubility, and the susceptibility to being metabolised by certain enzymes (*e.g.* certain cytochrome P450 families [CYP3A] or UDP-Glucuronosyltransferases [UGT]). Gastrointestinal (GI) physiology such as gastric emptying time, pH profiles, small intestinal transit time, abundance and genotype of gut wall drug metabolising enzymes and transporters can also affect f_a and F_G (Rowland and Tozer, 1989; Jamei *et al.*, 2009b).

Gastric emptying time can serve as the rate limiting step for highly permeable and highly soluble drugs as the absorption from the stomach is inevitably low (Higaki *et al.*, 2008). The gastrointestinal pH may affect drug dissolution for drugs displaying a pK_a within the range of the GI pH fluctuations (Blum *et al.*, 1991; Avdeef, 2007).

Furthermore, small intestinal transit time may influence the drug absorption of poorly soluble or extended release drug formulations as it is the main site of absorption (Koch *et al.*, 1993). Metabolism in the gut acts to regulate the oral bioavailability of drugs and other xenobiotics, an important determinant in the metabolism of substrate drugs (Kolars *et al.*, 1994). Cytochrome P450 (CYP), UDP-Glucuronosyltransferases, sulfotransferases (SULTs) and glutathione S-transferases (GST) drug metabolising enzymes are present in the enterocytes along the GI tract. CYP3A4 is the most abundant drug metabolising enzyme in the GI tract, preceding CYP2C9, CYP2C19, CYP2J2 and CYP2D6 in order of abundance (Peters *et al.*, 1989; Fisher *et al.*, 2001; Paine *et al.*, 2006; Riches *et al.*, 2009). CYP3A4 and CYP3A5 are both present along the whole GI tract, where CYP3A4 is expressed at lower levels in the duodenum, rising in the jejunum and decreasing towards the ileum (Kolars *et al.*, 1994; Paine *et al.*, 1997).

GI transporters may influence the absorption of orally administered drugs and potentially also the extent of metabolism in the gut through active substrate efflux (Benet and Cummins, 2001; Darwich *et al.*, 2010). Numerous transporters are present in the gut, such as the multidrug resistance transporter 1 (MDR1), also referred to as P-glycoprotein (P-gp), multidrug resistance associated protein 2 (MRP2) and breast cancer related protein (BCRP) (Fromm *et al.*, 2000; Maliepaard *et al.*, 2001). P-gp is the most extensively studied of the GI transporters and the relative expression pattern of P-gp in the small intestine increases from the proximal to the distal parts of the small intestine (Mouly and Paine, 2003).

The ADAM (Advanced Dissolution Absorption and Metabolism) model is a mechanistic representation of the GI tract which is implemented in the Simcyp[®] Simulator (Jamei *et al.*, 2009a). It is a successive development of the Advanced Compartmental Absorption and Transit (ACAT) model (Agoram *et al.*, 2001; Huang *et al.*, 2009), and includes distinct parameters which reflect the physiology better with regards to handling of fluid dynamics (no constant volume in each segment), anatomical mirroring of the GI anatomy and biology for different segments (un-equal segments with relative abundance of enzymes), and dissolution models (avoiding assumptions of a flat surface in Noyes-Whitney). The model defines the amount of drug in ‘formulation’, ‘released but undissolved’, ‘dissolved’ and ‘enterocytes’ as separate compartment structures and further adds hepato-biliary circulation and bile mediated solubility (Figure 1.4). The model also incorporates fluid dynamics along the GI tract flowing at the rate of gastric emptying and small intestinal transit time and rates of fluid absorption, secretion and reabsorption along the GI tract as opposed to a static volume in each segment (Jamei *et al.*, 2009b).

Furthermore, the ADAM model incorporates the abundance and distribution of GI enzymes and inter-individual variability as well as the distribution of the GI transporter P-gp (Jamei *et al.*, 2009b). The model attributes can be modified to reflect changes following bariatric surgery in a morbidly obese patient population and to investigate the validity of predicting the influence of surgery on oral bioavailability of drugs (Ghobadi *et al.*, 2011).

attributes of drugs or simplified categorisations such as the biopharmaceutics classification system (BCS) have been unsuccessful (Darwich *et al.*, 2012).

In the absence of clinical studies showing direction and magnitude of changes in bioavailability of various drugs, evidence-based mechanistic pharmacokinetic *in silico* models which define such alterations would be of value in determining appropriate dosage regimens for an increasing patient population who are undergoing bariatric surgery. The current study, to our knowledge, is the first to develop such a model.

3.3 Methods

3.3.1 Characterisation of post bariatric surgery population

A set of gastrointestinal and ‘whole body’ physiological parameters were identified based on factors influencing oral drug bioavailability post bariatric surgery, these included: gastric volume and gastric emptying rate, gastrointestinal pH, post surgical small intestinal dimensions, small intestinal motility and transit time and bile properties. Whole body physiological factors known to influence oral drug exposure were also identified, such as: renal function and serum protein levels as a function of post surgical weight loss.

An extensive literature search of identified parameters in relation to bariatric surgery was performed utilising PubMed (1966-2011). The gastrointestinal and physiological parameters were analysed in accordance to appropriate functions. Weighted means (WX) and standard deviations (overall SD) of results were calculated from the reported means (\bar{x}) and standard deviations (SD), dependent on the number of observations in the i^{th} study (n) (Equation 3.1, Equation 3.2 and Equation 3.3), and where applicable analysed using Welch’s t test at a significance level of 0.05 assuming parameter data to be normally distributed and taking unequal variance (s) into account, where \bar{X} is the sample mean and N is the sample size (Equation 3.4).

$$WX = \frac{\sum_{i=1}^n n_i \cdot x_i}{\sum_{i=1}^n n_i}$$

Equation 3.1. Calculating weighted mean.

$$OverallSD = \sqrt{\frac{Overall\ sum\ of\ squares}{N}}$$

Equation 3.2. Overall standard deviation.

$$Overall\ sum\ of\ squares = \sum_{i=1}^n \left[\left\{ (SD_i)^2 + (x_i)^2 \right\} \cdot n_i \right] - N \cdot WX^2$$

Equation 3.3. Overall sum of squares.

$$t = \frac{X_1 - X_2}{\sqrt{\frac{s_1^2}{N_1} + \frac{s_2^2}{N_2}}}$$

Equation 3.4. Welch's t test.

3.3.2 Adapting the ADAM model to mimic post bariatric surgery conditions

The Simcyp[®] Simulator v10 (Simcyp Ltd, Sheffield, UK) population template for Morbidly Obese based on a Northern European Caucasian population was used. Validation of this model with respect to prediction of clearance has recently been published by Ghobadi and co-workers (2011). We re-evaluated and analysed model performance against the identified post bariatric surgery model. Whenever applicable, we altered necessary population parameters to conform to post bariatric surgery conditions, applying reported data of weighted means and coefficient of variation (CV %) (Table 3.1).

Table 3.1. Pre- to post-surgery intrinsic factors.

Gastric emptying of liquids (minutes)
Gastric emptying of solids (minutes)
Post operative gastric volume (mL)
Secretion in stomach (Q_{sec} ; L/h)
Initial volume of stomach fluid (mL)
Small intestinal bypass (cm)
Small intestinal bile delay (cm)
Small intestinal bile concentrations at fasted and fed state (nM)
Gastrointestinal pH at fasted and fed state
GI CYP3A4 abundance (nmol/total gut)
GI CYP3A5 abundance (nmol/total gut)
Small intestinal transit time (hours)
Renal function (GFR; mL/min)
Human Serum Albumin levels (HSA; g/L)
α -1 Acid Glycoprotein levels (AGP; g/L)
Hepatic function (enzymatic activity)

GI=Gastrointestinal.

GFR=Glomerular filtration rate.

Post bariatric surgery gastrointestinal physiological parameters based on population/surgical data or physiologically rational assumptions were implemented to the ADAM model, creating ‘Post sleeve gastrectomy’, ‘Post Roux-en-Y gastric bypass’, ‘Post biliopancreatic diversion with duodenal switch’ and ‘Post jejunoileal bypass’ population templates (so called “population files” within Simcyp).

Post surgical basal steady state gastric fluid volumes at fasted state were estimated through one compartmental simulations of gastric fluid dynamics (Equation 3.5) in Matlab[®] R2010a (MathWorks, Natick, MA, USA) utilising reported post surgical gastric emptying and assuming a linear relationship with regards to the excretion of gastric juices (0.08 L/h) as a function of gastric capacity, utilising an average gastric volume of 230±13 mL as reported in 134 individuals. Saliva production was kept constant at 0.05 L/h (Valentin, 2002; Delgado-Aros *et al.*, 2004; Jamei *et al.*, 2009b).

$$\frac{dV_{st}}{dt} = Q_{sec,s} - k_{t,st} V_{st}$$

Equation 3.5. Gastric fluid dynamics model.

Population implementations of small intestinal bypass and delay in bile inlet were dimensionally estimated as a function of body surface area utilising Equation 3.6 and Equation 3.7, as implemented in the Simcyp® Simulator ADAM model. Further, the human effective permeability (P_{eff}) was set to close to zero in segments corresponding to the small intestinal bypass in the drug template (Turner, 2008).

$$Length\ of\ duodenum = 0.205 \cdot BSA^{0.550}$$

Equation 3.6. Length of the duodenum.

$$Length\ of\ jejunum\ and\ ileum = 5.231 \cdot BSA^{0.414}$$

Equation 3.7. Length of the distal small intestine.

Post surgical estimations of small intestinal transit time were implemented into the ADAM model utilising the incorporated Weibull distribution fitted to describe a log normal distribution through altering the scale factor (β) of small intestinal transit time keeping the shape factor (α) constant, altering β thus retaining the log normal distribution assumption (Equation 3.8) (Turner, 2008).

$$f(x) = \frac{\alpha}{\beta} \left(\frac{x}{\beta} \right)^{\alpha-1} e^{-(x/\beta)^\alpha}$$

Equation 3.8. Weibull distribution of variance in small intestinal transit.

Following the dimensional alterations to the post-operative surgical GI anatomy the bariatric surgical team at Salford Royal Foundation NHS Hospital Trust (Salford, UK) was consulted in order to establish consensus on physiological dimension reflecting a realistic patient population. The parameters subject to a consensus discussion included: Post surgical gastric volume and capacity, small intestinal bypass and delay in bile inlet.

3.3.3 *Virtual study of bioavailability ‘post bariatric surgery’*

An identified set of compounds in the Simcyp® Simulator were simulated utilising ‘Post Sleeve Gastrectomy in Morbidly Obese’, ‘Post Roux-en-Y Gastric Bypass in Morbidly Obese’, ‘Post Biliopancreatic Diversion with Duodenal Switch in Morbidly Obese’ and ‘Post Jejunioileal Bypass in Morbidly Obese’ population templates in a total of 100 subjects per group, displaying an age range of 20 to 50 years and 0.50 proportion of females, varying the mean small intestinal transit time to account for any ambiguity in reported data following surgery.

The selected drugs (simvastatin, omeprazole, diclofenac, fluconazole and ciprofloxacin) had a wide range of physicochemical and metabolic attributes and were commonly used in patients undergoing bariatric surgery (Darwich *et al.*, 2012). Oral drug exposure was simulated for a low, medium and high therapeutic dose in accordance with the British National Formulary (BNF), which included: Simvastatin immediate release (IR; 10, 20 and 80 mg), diclofenac enteric-coated (EC; 25, 50 and 75 mg), omeprazole EC (10, 20 and 40 mg), fluconazole IR (50, 200, 400 mg) and ciprofloxacin IR (250, 500 and 750 mg). Drugs simulated in post bariatric surgery population templates were compared to simulations carried out in the Morbidly Obese population template, examining trends in oral drug bioavailability, f_a and F_G (Equation 1.1), and related surrogate biomarkers: AUC_{0-24h} , C_{max} and t_{max} where simulated data were analysed in MATLAB® R2010a.

3.4 Results

3.4.1 *Characterisation and validation of virtual populations*

Roux-en-Y gastric bypass (RYGB)

Post RYGB stomach volume:

A reduced gastric volume was implemented in the ‘Morbidly Obese’ population template through limiting concomitant fluid intake from the default value of 250 mL to 30 mL based on surgical restriction in accordance to Wittgrove and Clark (2000). The initial volume of stomach fluid at fasted state was estimated to be 9.9 mL (CV: 30%) utilising simulations at steady state as per Equation 3.5.

Gastric acid secretion and pH:

Two studies were identified measuring gastric acid production in a total of 18 post RYGB patients, with an approximate gastric volume of 10 mL, as compared to pre surgery or controls (Smith *et al.*, 1993; Behrns *et al.*, 1994). Combining weighted means and variance displayed a mean basal gastric acid excretion of 0.08 (± 0.008) mEq/h, and a weighted mean peak acid excretion of 0.048 (± 0.048) mEq/30 minutes post surgery, as compared to a basal and peak acid excretion of 9.1 ± 3.6 mEq/h ($P < 0.05$) and 12.8 ± 1.8 mEq/30 minutes ($P < 0.05$) respectively in pre surgery patients (n=8) and a basal and peak acid secretion of 5.0 ± 0.7 ($P < 0.05$) and 12.1 ± 1.3 ($P < 0.05$) respectively in healthy volunteers (n=15) (Figure 3.2) (Smith *et al.*, 1993; Behrns *et al.*, 1994).

Implementation into the Simcyp[®] Simulator Morbidly Obese population template was based on assuming a gastric pH of 6.4 at fasted state.

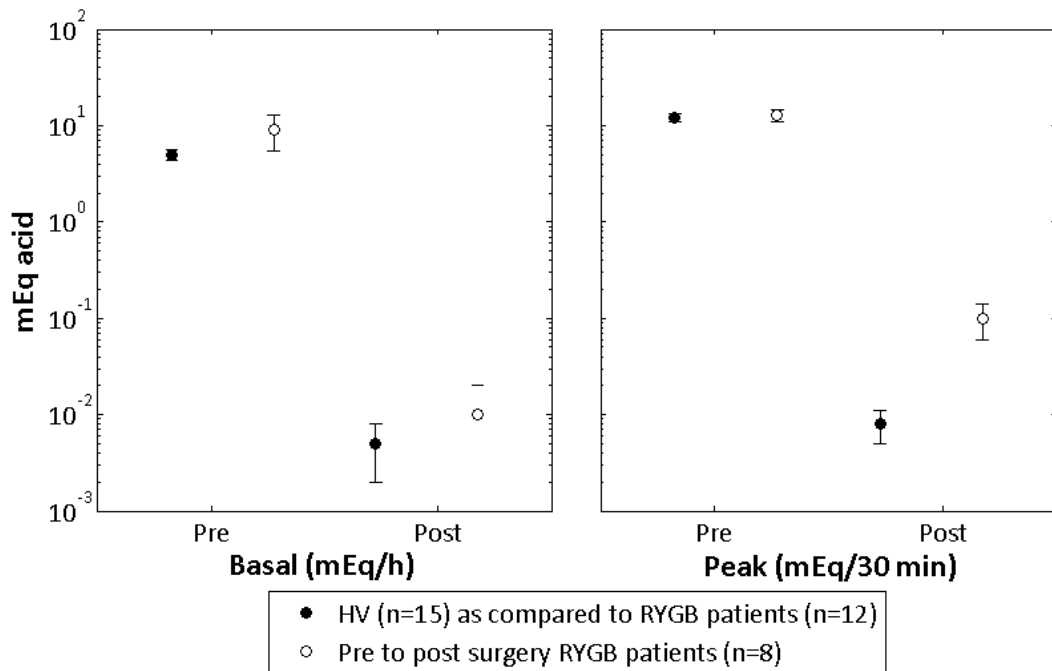


Figure 3.2. Mean acid secretion and standard deviation, mEq HCl, over time at basal and peak level. Acid secretion in 12 post Roux-en-Y Gastric Bypass (RYGB) patients as compared to 15 healthy volunteers not subject to surgery (HV) (Smith *et al.*, 1993). Acid secretion in 8 RYGB patients, pre and post surgery (Behrns *et al.*, 1994).

Gastric emptying time:

Following RYGB surgery a significant reduction in $t_{1/2}$ gastric emptying time has been observed for liquids, whereas available data on gastric emptying of solids display a considerably increased variability (Figure 3.3 and Figure 3.4). Four studies measuring gastric emptying time following gastrectomy surgery were identified (RYGB, SG, Billroth gastrectomy with Roux-en-Y gastrectomy and partial gastrectomy). Combining weighted means and variance in a total of 68 post surgery patients resulted in a mean $t_{1/2}$ gastric emptying of 8.48 (± 9.12) minutes, as compared to 24.33 (± 23.71) minutes in controls (n=39; $P < 0.05$) (Figure 3.3). (Horowitz *et al.*, 1982; Hinder *et al.*, 1988; Rieu *et al.*, 1989; Braghetto *et al.*, 2009)

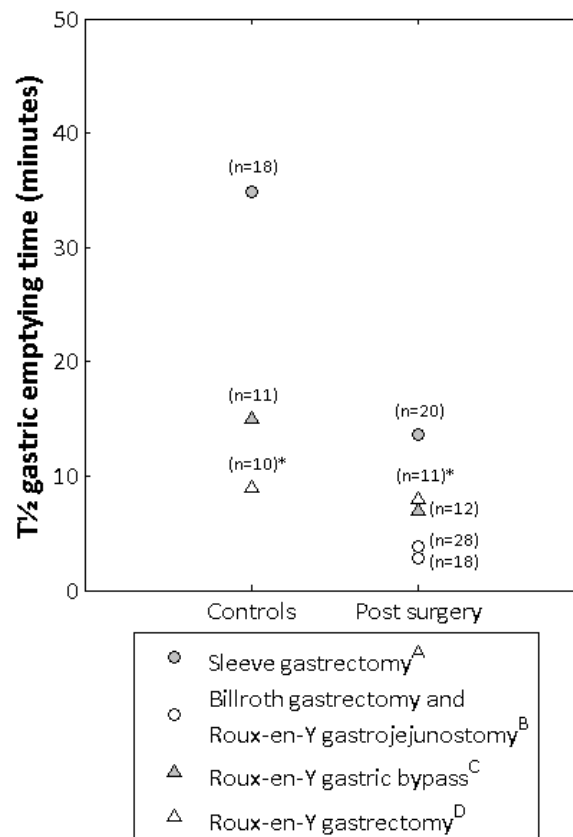


Figure 3.3. Reported mean (*median) $t_{1/2}$ gastric emptying time of liquids in post gastric surgery patients subject to various surgeries resulting in a reduced gastric volume as compared to controls (pre surgery or healthy volunteers not subject to surgery). A: Sleeve gastrectomy, B: Billroth gastrectomy and Roux-en-Y gastrojejunostomy, C: Roux-en-Y gastric bypass and D: Roux-en-Y gastrectomy (Horowitz *et al.*, 1982; Hinder *et al.*, 1988; Rieu *et al.*, 1989; Braghetto *et al.*, 2009).

Identified publications examining gastric emptying time of solids post gastric surgery resulting in a reduced gastric volume (RYGB, SG and Billroth gastrectomy with Roux-en-Y gastrectomy) displayed an observable increase in variability following surgery as compared to controls: reported observations ranging from 4 minutes to over 200 minutes post surgery (Figure 3.4) (Shah *et al.*, 2010; Horowitz *et al.*, 1982; Hinder *et al.*, 1988; Rieu *et al.*, 1989; Petrakis *et al.*, 1998; Bernstine *et al.*, 2009; Braghetto *et al.*, 2009).

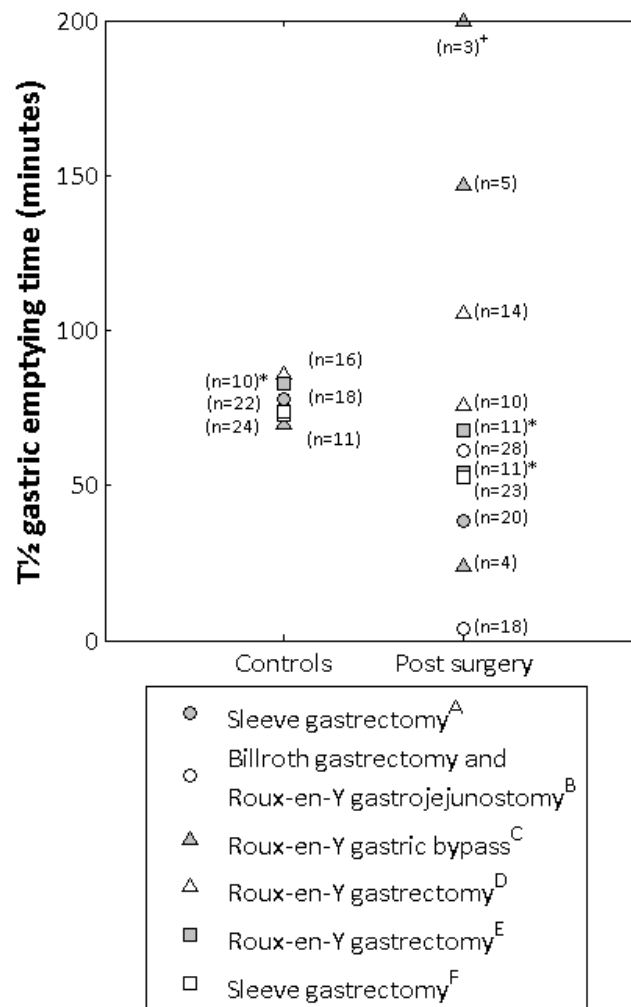


Figure 3.4. Reported mean (*median) $t_{1/2}$ gastric emptying time of solids in post gastric surgery patients subject to various gastrointestinal surgeries, as described in publication, resulting in a reduced gastric volume as compared to controls. A: Sleeve gastrectomy, B: Billroth gastrectomy and Roux-en-Y gastrectomy, C: Roux-en-Y gastric bypass, D: Roux-en-Y gastrectomy, E: Roux-en-Y gastrectomy, F: sleeve gastrectomy (Shah *et al.*, 2010; Horowitz *et al.*, 1982; Hinder *et al.*, 1988; Rieu *et al.*, 1989; Petrakis *et al.*, 1998; Bernstine *et al.*, 2009; Braghetto *et al.*, 2009).

Following RYGB, the gastric emptying half-life of liquids was measured to be 7 (± 3) minutes after liquid intake in 12 post gastric bypass patients 12 months post surgery with a newly formed stomach pouch of size of 60-80 mL and a gastrojejunal anastomosis of 12-20 mm in diameter, as compared to 11 healthy volunteers displaying a gastric emptying half-life of 15 (± 2) minutes (Figure 3.3) (Horowitz *et al.*, 1982).

Gastric emptying half-life of a solid meal was highly variable in the post RYGB patient population, where 4 patients displayed a $t_{1/2}$ of 24 (± 10) minutes, exhibiting an initial rapid gastric emptying followed by a linear emptying, whereas five patients displayed an initial lag time followed by linear emptying. Three patients displayed a prolonged lag time followed by slow gastric emptying, with a reported gastric emptying half time of over 200 minutes. The control group displayed a $t_{1/2}$ of 70 (± 7) minutes (Figure 3.4). Alteration to the gastric emptying was implemented based on post surgical gastric emptying time for liquids of 7 (CV: 45%) minutes in a fasted state (Horowitz *et al.*, 1982).

Small intestinal bypass and regional abundances of CYP3A:

Approximately 75-100 cm's of the proximal small intestine is bypassed following RYGB surgery, bypassing the duodenum and proximal jejunum (Wittgrove and Clark, 2000; DeMaria *et al.*, 2002; Schneider and Mun, 2005; Elder and Wolfe, 2007; Skottheim *et al.*, 2009; Spak *et al.*, 2010). In accordance with the small intestinal bypass, the duodenum and proximal jejunum were bypassed through setting transit time close to zero in the duodenum and reducing small intestinal transit time in jejunum I by 38%, thus creating an approximate bypass of 87.5 cm in the ADAM model based on BSA (Equation 3.6 and Equation 3.7).

Small intestinal motility and transit time:

Studies in humans examining small intestinal transit and motility in patients subject to total gastrectomy were reviewed, as compared to a partial gastrectomy in the treatment of obesity (Pellegrini *et al.*, 1986; Haglund *et al.*, 1989; Le Blanc-Louvry *et al.*, 1999; Wittgrove and Clark, 2000).

The data suggested changes in small intestinal motility after a Roux-en-Y reconstruction (van der Mijle *et al.*, 1993; Le Blanc-Louvry *et al.*, 2000). In ten patients subject to Roux-en-Y with a total gastrectomy (cancer being the main indication), a mean small intestinal transit for solids of 293 (± 37) minutes was observed as compared to 187 (± 37) minutes in five controls ($P < 0.02$), thus suggesting the small intestinal transit to be increased post Roux-en-Y gastric bypass (Pellegrini *et al.*, 1986). Animal models of Roux-en-Y gastric bypass surgery suggested a similar impact of surgery as that observed in man, with disturbed small intestinal motility reported in rat and dog (Woodward *et al.*, 1993; Le Blanc-Louvry *et al.*, 1999; Suzuki *et al.*, 2005).

Two scenarios were created with regards to small intestinal transit time. In the first scenario the transit time was assumed to be 5.0 hours based on a reduced motility as reported by Pellegrini and co-workers (1986); whereas, in the second scenario the small intestinal motility was assumed to remain unaltered thus reducing small intestinal transit to 3.0 hours as a function of the small intestinal bypass (Pellegrini *et al.*, 1986).

Regional abundances of CYP3A metabolising enzymes were set to close to zero in the bypassed segments of the small intestine. Mean total enzyme abundances of CYP3A4 and CYP3A5 were recalculated to account for the small intestinal bypass of the duodenum, resulting in a reduction from 66.2 to 50.2 nmol/total gut and from 24.6 to 18.7 nmol/total gut respectively (Turner, 2008).

Bile and pancreatic fluids

Following RYGB surgery, the inlet of bile and pancreatic fluids is delayed to the common channel approximately 75-150 cm distally of the newly formed stomach pouch (Wittgrove and Clark, 2000; DeMaria *et al.*, 2002; Spak *et al.*, 2010). A delayed bile inlet was implemented into the ADAM model through setting bile concentrations in the fasted and fed state to zero in the gastrointestinal regions of the stomach, duodenum and jejunum corresponding to approximately 90 cm.

Biliopancreatic diversion with duodenal switch (BPD-DS)

Stomach volume

In accordance to the surgical procedure the gastric volume following biliopancreatic diversion with duodenal switch was effectively restricted to 150 mL, through limiting concomitant fluid intake with oral administration to 150 mL. Due to lack of data gastric emptying and gastric pH was assumed to remain unaltered (Smith *et al.*, 1993; Behrns *et al.*, 1994; Wittgrove and Clark, 2000; DeMaria *et al.*, 2002; Schneider and Mun, 2005; Elder and Wolfe, 2007; Spak *et al.*, 2010).

Small intestinal bypass and regional abundances of CYP3A:

Segments Jej1 and 2 were bypassed corresponding to approximately 294 cm (Wittgrove and Clark, 2000); recalculating gastrointestinal abundances of CYP3A4 and CYP3A5 accordingly to 30.0 and 11.2 nmol/total gut respectively (Turner, 2008).

Small intestinal motility and transit time:

In the first scenario the transit time was assumed to be 3.7 hours in accordance to the reduced motility observed post total gastrectomy with Roux-en-Y jejunostomy corrected for the small intestinal length following BPD-DS (Pellegrini *et al.*, 1986); whereas, in the second scenario the small intestinal motility was assumed to be 2.2 hours thus reducing as a function of the small intestinal bypass.

Bile and pancreatic fluids

In accordance with the surgical procedure the bile inlet was delayed to ileum III corresponding to 252 cm (Wittgrove and Clark, 2000; Schneider and Mun, 2005; Elder and Wolfe, 2007).

Sleeve gastrectomy (SG)

Stomach volume:

Sleeve gastrectomy surgery is limited to the restriction of the dimension of the gastric pouch (to approximately 60-80 mL), preserving the pyloric sphincter (Baltasar *et al.*, 2005; Lee *et al.*, 2007). Albeit not being as invasive as malabsorptive procedures, the reduction in gastric volume has been reported to affect the gastric emptying time of liquids and solids (Figure 3.2 and Figure 3.3) (Braghetto *et al.*, 2009; Shah *et al.*, 2010). This was implemented through setting concomitant fluid intake to 80 mL and initial

volume of stomach fluid to 24.2 mL (CV: 30%) in the fasted state in accordance with simulated steady state gastric volumes.

Gastric emptying time

One study was identified examining gastric emptying of liquids following sleeve gastrectomy, observing a significantly reduced $t_{1/2}$ gastric emptying time of 13.6 (± 11.9) minutes in 20 post surgery patients as compared to 34.9 (± 24.6) minutes in 18 controls (Figure 3.3) (Braghetto *et al.*, 2009). Thus, gastric emptying was set to 13.6 (CV: 53%) in the post sleeve gastrectomy population template.

Results from combining weighted means and variance of identified studies examining gastric emptying of solids resulted in a significant reduction post operatively ($P < 0.05$), with an observed mean gastric emptying time of 46.1 (± 17.7) minutes in 43 post surgery patients as compared to 74.6 (± 26.2) minutes in 64 controls (Figure 3.4) (Braghetto *et al.*, 2009; Shah *et al.*, 2010)

Gastric acid secretion and pH:

There is a lack of published data on the impact of sleeve gastrectomy on gastric acid secretion or gastric pH measurements pre to post surgery. Given this, gastric pH was assumed to remain unaltered following sleeve gastrectomy.

Jejunioileal bypass (JIB)

Small intestinal bypass and regional abundance of CYP3A:

In accordance with the surgical procedure a small intestinal bypass was created retaining the duodenum segment, 20% of the proximal jejunum I and 23% of the terminal ileum IV approximately, bypassing the remainder of the small intestine (Scott *et al.*, 1971; Scott *et al.*, 1973; Griffen *et al.*, 1977). Accordingly the abundances of CYP3A4 and CYP3A5 were set to zero in jejunum II to Ileum III and recalculated to 32.3 and 12.1 nmol per total gut respectively.

Small intestinal motility and transit time:

In the first scenario the transit time was assumed to be 0.7 hours in accordance to the reduced motility observed post total gastrectomy with Roux-en-Y jejunostomy corrected for the small intestinal length post JIB; whereas, in the second scenario the

small intestinal motility was assumed to be 0.4 hours thus reducing as a function of the small intestinal bypass (Pellegrini *et al.*, 1986).

Bariatric surgery – Whole body physiological parameters

Renal function:

Comparing observed data on renal function, in terms of Glomerular Filtration Rate (GFR), in relation to BMI following bariatric surgery induced weight loss, estimates made utilising Cockcroft-Gault and Modification of Diet in renal Disease (MDRD; Equation 3.9) equations, concluded a better prediction by MDRD equation (Chagnac *et al.*, 2003; Navarro-Diaz *et al.*, 2006; Serra *et al.*, 2006; Saliba *et al.*, 2010). The Cockcroft-Gault equation estimates the creatinine clearance the MDRD equation estimates the GFR corrected for body surface area (Michels *et al.*, 2010). Simulating age and sex matched populations over a range of BMI, utilising the Simcyp[®] Simulator incorporating inter-individual variability, observed data was within 95% confidence interval of simulated estimations utilising the MDRD equation, whereas, Cockcroft Gault over predicted GFR at a higher BMI in agreement with previous publications examining predicted versus observed GFR in Morbidly Obese and Obese populations (Figure 3.5) (Michels *et al.*, 2010; Ghobadi *et al.*, 2011). Based on these findings the MDRD equation was utilised to estimate GFR in the Simcyp[®] Simulator.

$$GFR(mL/min/1.73m^2) = 186 \cdot Serumcreatinine^{-1.154} \cdot age^{-0.203} \cdot (0.742 \text{ for females})$$

Equation 3.9. Modification of Diet in renal disease (MDRD) equation for estimating glomerular filtration rate (GFR).

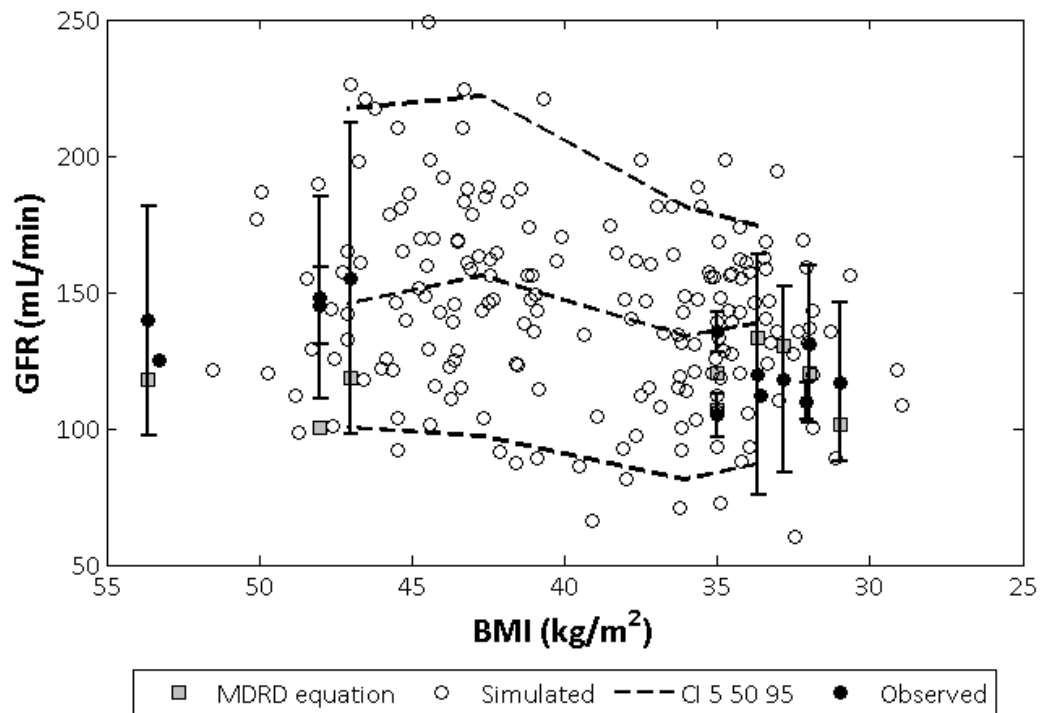


Figure 3.5. Observed Glomerular Filtration Rate (GFR) following bariatric surgery induced weight loss, as compared to calculated GFR utilising the Modification of Diet in Renal Disease (MDRD) equation and simulated age and gender matched GFR with 5, 50 and 95% confidence intervals (CI) utilising the Simcyp[®] Simulator (MDRD) with inter-individual variability (Chagnac *et al.*, 2003; Navarro-Diaz *et al.*, 2006; Serra *et al.*, 2006; Saliba *et al.*, 2010).

Serum protein levels:

Prior to and following bariatric surgery induced weight loss, Human Serum Albumin (HSA) levels remained consistent with the normal reported range (at a total of 322 data points; n=163) evaluated utilising sex and age matched simulations in the Simcyp[®] Simulator, predicting HSA within the 95% confidence interval (Figure 3.6) (Benedek *et al.*, 1984; Mattar *et al.*, 2005; Stratopoulos *et al.*, 2005; Barker *et al.*, 2006). Levels of α -1 Acid Glycoprotein (AGP) was significantly reduced following bariatric surgery induced weight loss (at a total of 170 data points; n=50), regressing towards ranges observed in normal weight controls, where simulations in Simcyp[®] Simulator overestimated the levels of AGP at lower BMI ranges (Figure 3.7) (Benedek *et al.*, 1984; van Dielen *et al.*, 2004).

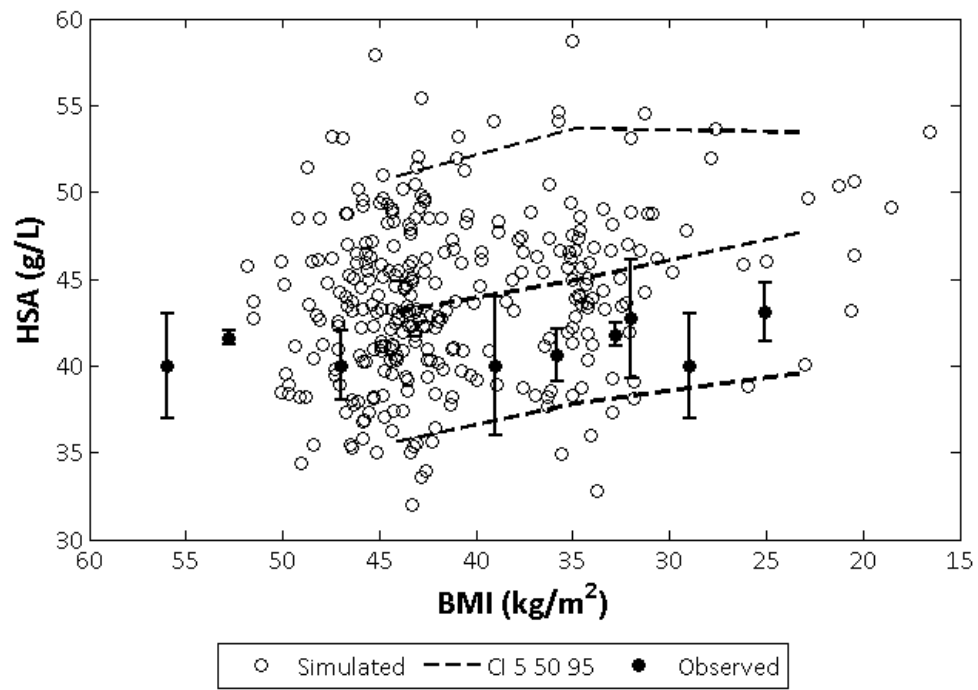


Figure 3.6. Observed mean and standard deviation of serum concentrations of Human Serum Albumin (HSA) in morbidly obese patients subject to bariatric surgery induced weight loss as compared to simulated HSA levels with 5, 50 and 95% confidence intervals (CI) based on Simcyp[®] demographics characteristics (Benedek *et al.*, 1984; Mattar *et al.*, 2005; Stratopoulos *et al.*, 2005; Barker *et al.*, 2006).

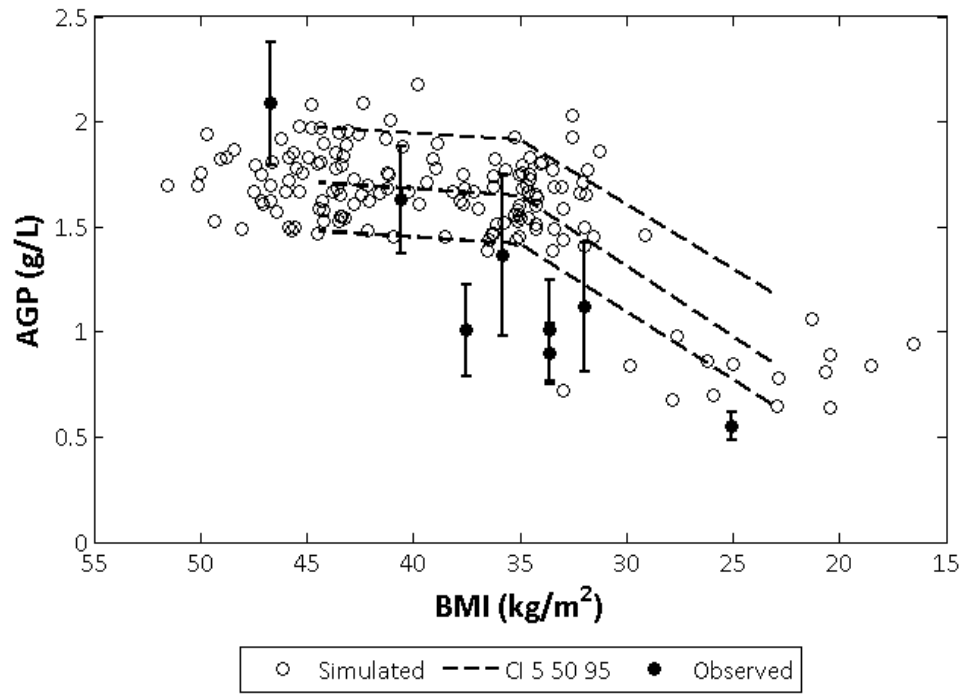


Figure 3.7. Observed mean and standard deviation of serum concentrations of α -1 Acid Glycoprotein (AGP) in morbidly obese patients subject to bariatric surgery induced weight loss as compared to simulated AGP levels with 5, 50 and 95% confidence intervals (CI) based on Simcyp[®] Simulator demographics characteristics (Benedek *et al.*, 1984; Mattar *et al.*, 2005; Stratopoulos *et al.*, 2005; Barker *et al.*, 2006).

Hepatic function:

The reduction in liver volume following bariatric surgery induced weight loss was assumed to be a function of the reduction in Body Surface Area (BSA) as observed in a general population, where the equation incorporated into the Simcyp[®] Simulator corrects for the observed under prediction in liver volume at a BMI ≥ 40 kg/m² utilising a correction factor of 1.25 (Johnson *et al.*, 2005; Ghobadi *et al.*, 2011). Tissue blood perfusions were obtained as a function of cardiac output estimated from BSA as incorporated into the Simcyp[®] Simulator (Howgate *et al.*, 2006).

Table 3.2. Summary of physiological parameters alterations following bariatric surgery for input into Simcyp® Simulator.

Physiological parameters	RYGB	BPD-DS	JIB	SG	References
Population alterations					
Stomach					
Gastric emptying time (h)	7.0 (CV 45%)	Unaltered	Unaltered	13.6 (CV 53%)	(Horowitz <i>et al.</i> , 1982; Braghetto <i>et al.</i> , 2009)
Initial fluid volume (mL)	9.9 (CV 30%)	Unaltered	Unaltered	24.2 (CV 30%)	
Gastric pH	6.4 (CV 38%)	1.5 (CV 38%)	1.5 (CV 38%)	1.5 (CV 38%)	(Smith <i>et al.</i> , 1993; Behrns <i>et al.</i> , 1994)
Small intestine					
Bypass (segments)	Duo, jej I†	Jej I, jej II	Jej II-II III	Unaltered	(Scott <i>et al.</i> , 1971; Scott <i>et al.</i> , 1973; Wittgrove and Clark, 2000; DeMaria <i>et al.</i> , 2002; Chagnac <i>et al.</i> , 2003; Baltasar <i>et al.</i> , 2005; Schneider and Mun, 2005; Navarro-Diaz <i>et al.</i> , 2006; Serra <i>et al.</i> , 2006; Elder and Wolfe, 2007; Lee <i>et al.</i> , 2007; Skotheim <i>et al.</i> , 2009; Saliba <i>et al.</i> , 2010; Spak <i>et al.</i> , 2010)
Bile delay (segments)	Duo-jej I†	Duo-il II	Unaltered	Unaltered	
SIT: Scenario 1 (h)	3.0	2.2	0.4	3.3	
Weibull β^*	3.6	2.6	0.5	4.0	
SIT: Scenario 2	5.0	3.7	0.7	-	
Weibull β^*	6.0	4.4	0.8	-	
GI metabolism					
CYP3A bypass (segments)	Duo, jej I†	Jej I, jej II	Jej II-II III	Unaltered	
CYP3A4 abundance	50.2 (CV 60%)	30.0 (CV 60%)	32.3 (CV 60%)	66.2 (CV 60%)	
CYP3A5 abundance	18.7 (CV 60%)	11.2 (CV 60%)	12.1 (CV 60%)	24.2 (CV 60%)	
Whole-body physiology					
GFR prediction	MDRD	MDRD	MDRD	MDRD	
Study design alterations					
Fluid intake with dose	30 (CV 60%)	150 (CV 60%)	250 (CV 60%)	80 (CV 60%)	

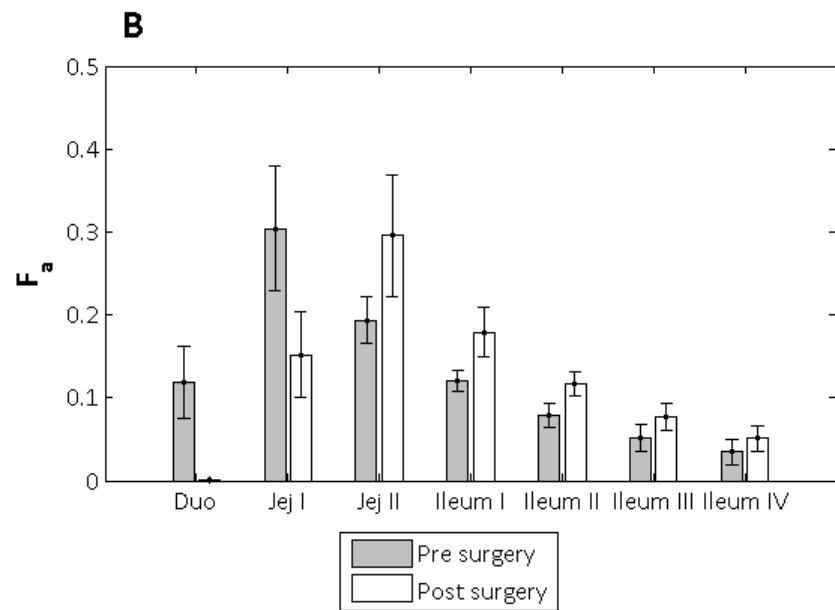
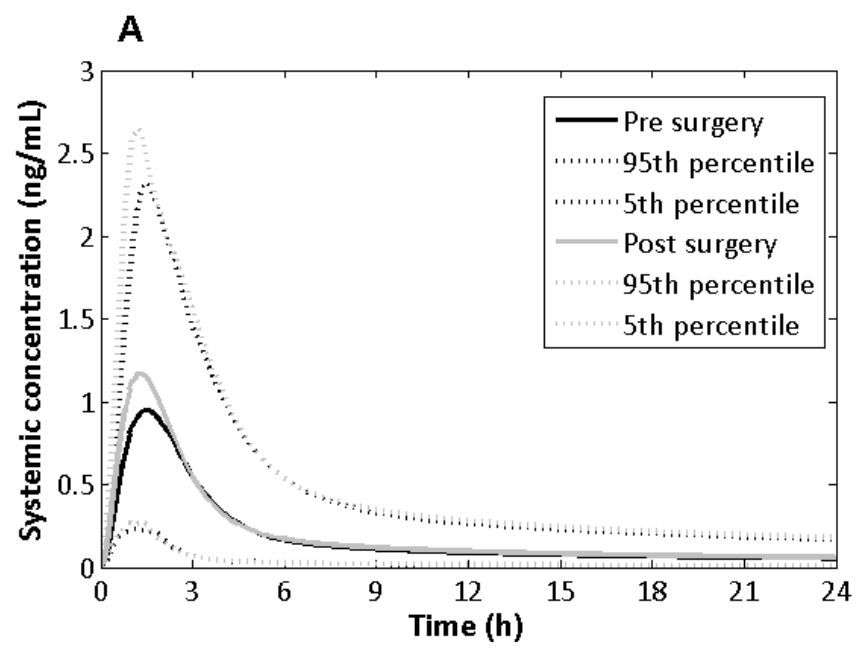
RYGB=Roux-en-Y gastric bypass, BPD-DS=biliopancreatic diversion with duodenal switch, JIB=jejunoileal bypass, SG=sleeve gastrectomy, SIT=small intestinal transit, GI=gastrointestinal, duo=duodenum, jej=jejunum, IL=ileum, GFR=glomerular filtration rate, MDRD=modification of diet in renal disease, Weibull function ($\alpha=2.92$; Equation 3.8). †Partial small intestinal bypass.

3.4.2 Virtual studies

Roux-en-Y gastric bypass:

Simulated simvastatin IR 10 mg oral drug exposure post RYGB (SIT=3.0h) displayed an unaltered oral bioavailability with a mean post/pre surgery AUC ratio of 1.14 ± 0.18 due to a mean increase in F_G from $0.24 (\pm 0.10)$ to $0.27 (\pm 0.11)$ counteracted by a reduction in f_a from $0.90 (\pm 0.11)$ to $0.87 (\pm 0.12)$ (Figure 3.8). At a high therapeutic dose (80 mg) the mean post/pre surgery ratio became less apparent (1.07 ± 0.19) due to a more apparent reduction in f_a from 0.88 ± 0.12 to 0.82 ± 0.14 (Figure 3.9). Assuming a reduction in small intestinal motility post RYGB (SIT=5.0h) simvastatin displayed a mean ratio of $1.22 (\pm 0.19)$ to $1.17 (\pm 0.20)$ over the therapeutic dose range due to reduced post operative impact on f_a . This was apparent over the whole range of studied drugs, where the increased small intestinal transit time influenced f_a positively (data not shown).

Oral drug exposure of omeprazole remained unaltered following RYGB (SIT=3.0h), although displaying a reduction in t_{max} from approximately $1.24 (\pm 0.41)$ to $0.97 (\pm 0.23)$ hours over the therapeutic dose range. Diclofenac post/pre surgery AUC ratio displayed a minor reduction following RYGB (SIT=3.0h). This became more apparent at a high therapeutic dose, displaying an AUC ratio of $0.99 (\pm 0.14)$, due to a reduction in f_a $0.88 (\pm 0.13)$ to $0.84 (\pm 0.13)$, counteracted by a minor increase in F_G from $0.95 (\pm 0.04)$ to $0.96 (\pm 0.03)$; whereas t_{max} displayed a reduction from $1.44 (\pm 0.54)$ to $1.28 (\pm 0.51)$ hours. Ciprofloxacin displayed a minor reduction in AUC post RYGB (SIT=3.0h), displaying a ratio of $0.96 (\pm 0.02)$ over the therapeutic dose range due to a reduction in f_a from $0.77 (\pm 0.15)$ to $0.74 (\pm 0.15)$. Fluconazole remained unaltered over the dose range.



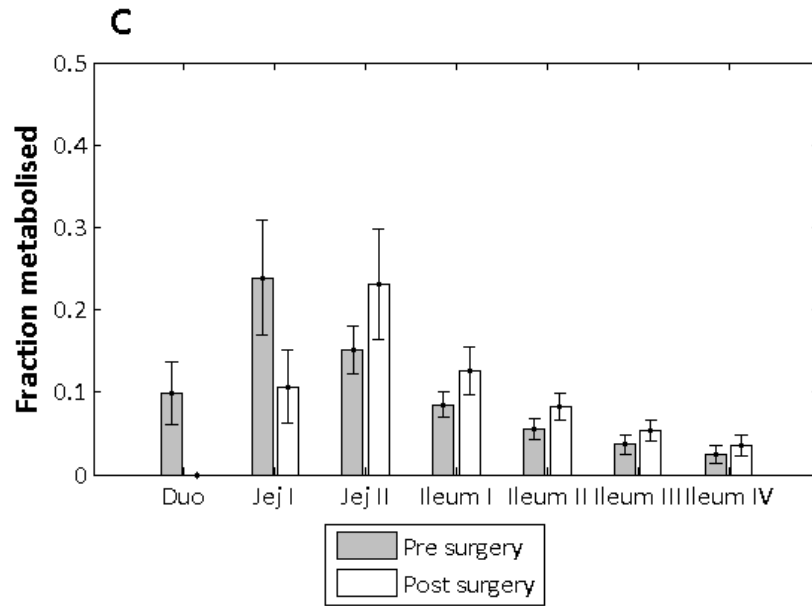


Figure 3.8. Simulated simvastatin immediate release (IR) 10 mg (low therapeutic dose) in morbidly obese (n=100) and post Roux-en-Y gastric bypass surgery (n=100; small intestinal transit=3.0h) **A:** Mean, 95th and 5th percentile plasma concentration time profile over 24 hours, **B:** Mean and standard deviation of segmental fraction of dose absorbed along the small intestine (f_a), **C:** Mean and standard deviation of segmental fraction of dose metabolised in the gut wall ($1-F_G$). Duo=duodenum, Jej=jejunum.

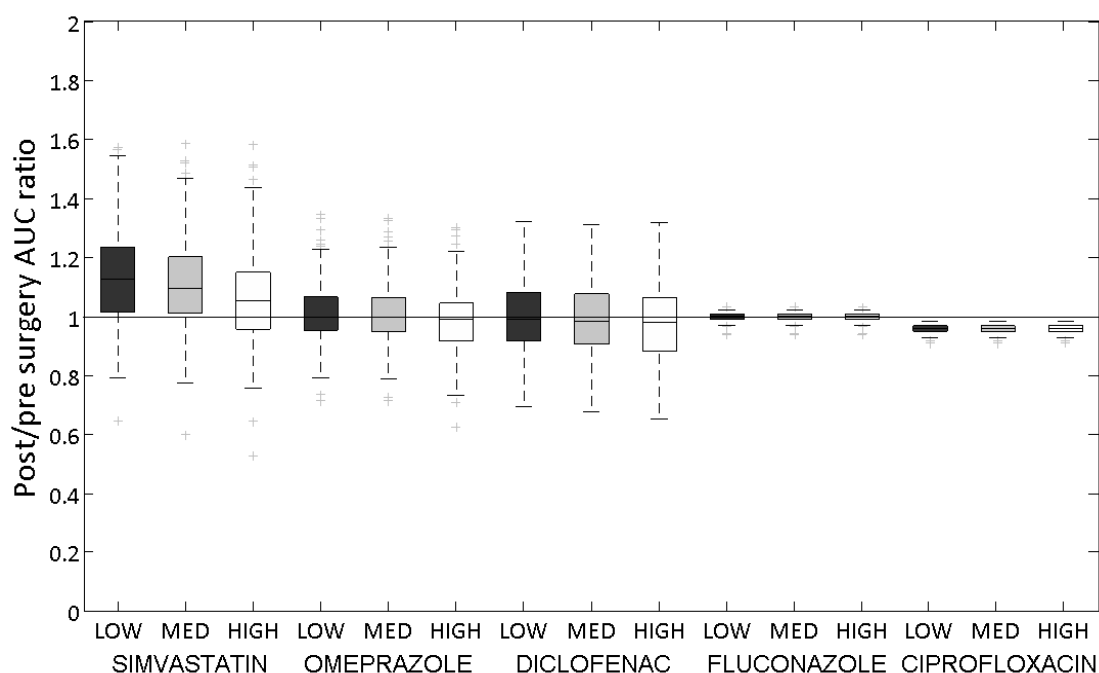


Figure 3.9. Simulated post/pre Roux-en-Y gastric bypass surgery (small intestinal transit=3.0h) AUC ratio over a range of selected drugs at a low (LOW), medium (MED) and high (HIGH) therapeutic dose: Simvastatin immediate release (IR; 10, 20 and 80 mg), omeprazole enteric coated (EC; 10, 20 and 40 mg), diclofenac EC (25, 50 75 mg), fluconazole IR (50, 200, 400 mg) and ciprofloxacin IR (250, 500 and 750 mg).

Biliopancreatic diversion with duodenal switch:

Following BPD-DS (SIT=2.2 h), simvastatin displayed a reduction in AUC, with an observed post/pre surgical AUC ratio ranging from 0.89 (± 0.15) to 0.65 (± 0.22) as a result of a more extensive reduction in f_a as compared to following RYGB; whereas assuming a higher SIT of 3.7 h simvastatin displayed an increase in AUC, displaying a ratio of 1.05 (± 0.08) at a low therapeutic dose level ranging to a reduction, with a simulated ratio of 0.83 (± 0.22) at the highest therapeutic dose. This was observed for the whole range of simulated drugs.

Omeprazole displayed a post/pre BPD-DS AUC ratio of 0.88 (± 0.10) at a low therapeutic dose due to a reduction in f_a from 0.94 (± 0.09) to 0.83 (± 0.14) (Figure 3.10), whereas a minor increase in F_G was observed from 0.96 (± 0.02) to 0.97 (± 0.02). T_{max} displayed an increase from 1.22 (± 0.38) to 1.50 (± 0.54) hours, whereas C_{max} displayed a reduction by approximately 19%. At a high therapeutic dose, omeprazole displayed a

post/pre surgery AUC ratio of 0.77 (± 0.15), due to a more extensive reduction in f_a ; whereas t_{max} was increased from 1.42 (± 0.50) to 2.26 (± 0.63) hours. The reduction became less apparent assuming a small intestinal transit time of 3.7 h.

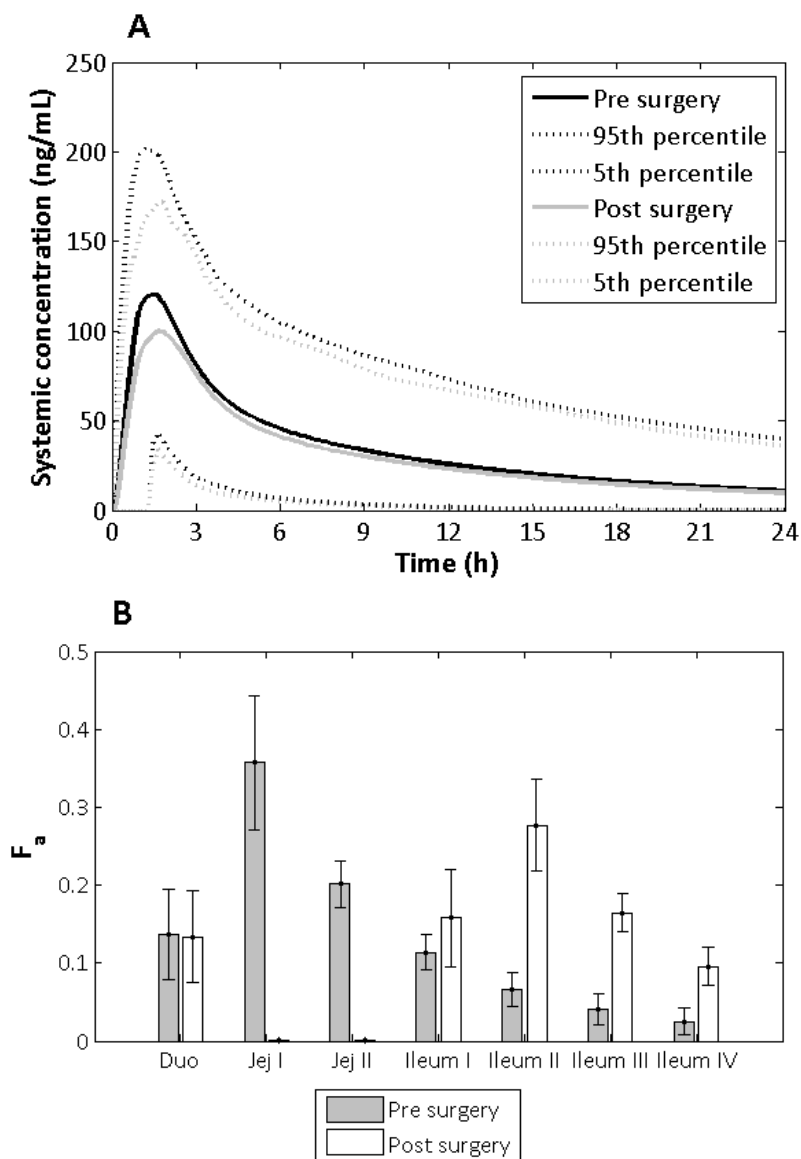


Figure 3.10. Simulated omeprazole enteric coated (EC) 10 mg (low therapeutic dose) in morbidly obese (n=100) and post biliopancreatic diversion with duodenal switch (n=100; small intestinal transit=2.2h) **A:** Mean, 95th and 5th percentile plasma concentration time profile over 24 hours, **B:** Mean and standard deviation of segmental fraction of dose absorbed along the small intestine (f_a). Duo=duodenum, Jej=jejunum.

Diclofenac displayed an AUC ratio of 0.87 (± 0.09) following BPD-DS (SIT=2.2 h) at a low therapeutic dose due to a reduction in f_a from 0.89 (± 0.12) to 0.75 (± 0.15), whereas F_G displayed an increase from 0.91 (± 0.06) to 0.94 (± 0.04). At a high therapeutic dose diclofenac displayed a more apparent reduction due to a higher post surgical impact on f_a . Again the reduction was less apparent assuming a small intestinal transit time of 3.7 h (Figure 3.11).

Fluconazole displayed an AUC ratio of approximately 0.95 (± 0.05) over the dose range. Ciprofloxacin displayed an AUC ratio of 0.80 (± 0.06) following BPD-DS (SIT=2.2 h) at a low therapeutic dose, reflected by a reduction in f_a . Following BPD-DS (SIT=3.7 h), Ciprofloxacin displayed no significant alteration, with an AUC ratio of 1.01 (± 0.01) at a low therapeutic dose ranging to 0.98(± 0.01) at a high therapeutic dose (Figure 3.11).

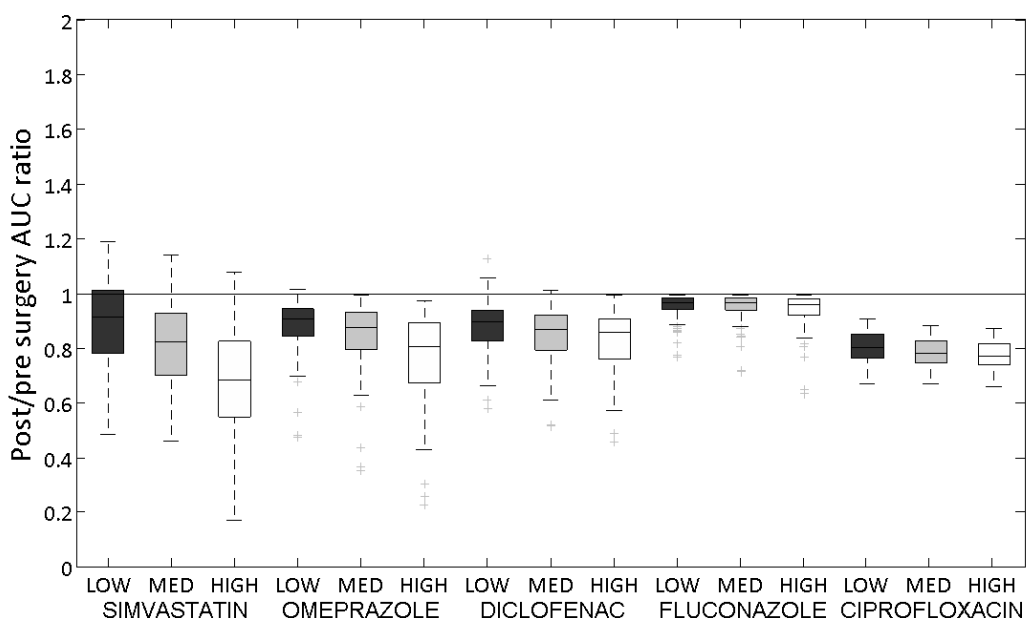
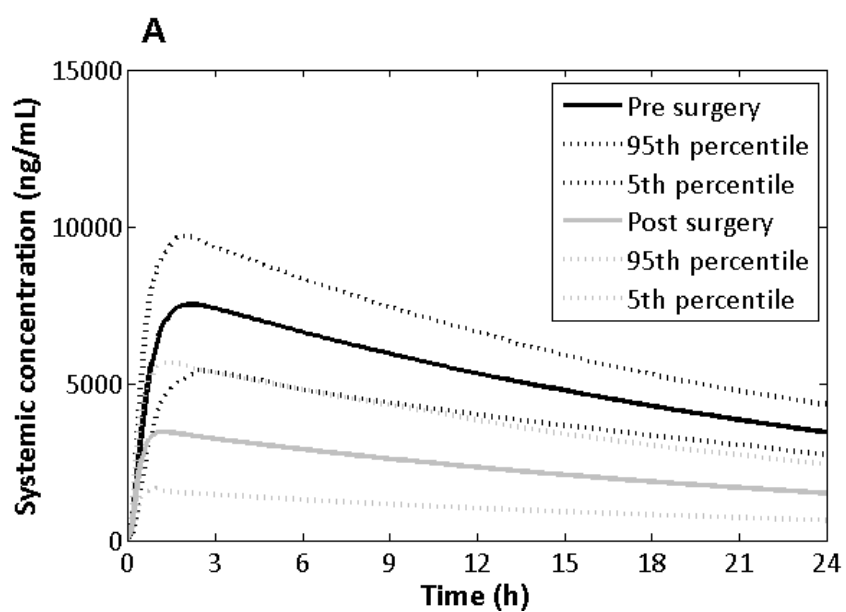


Figure 3.11. Simulated post/pre biliopancreatic diversion with duodenal switch (small intestinal transit=2.2h) AUC ratio over a range of selected drugs at a low (LOW), medium (MED) and high (HIGH) therapeutic dose: Simvastatin immediate release (IR; 10, 20 and 80 mg), omeprazole enteric coated (EC; 10, 20 and 40 mg), diclofenac EC (25, 50 75 mg), fluconazole IR (50, 200, 400 mg) and ciprofloxacin IR (250, 500 and 750 mg).

Jejunioleal bypass:

Following JIB the whole range of studied drugs displayed an extensive reduction in AUC due to a more apparent reduction in f_a as compared to RYGB and BPD-DS where fluconazole displayed the least apparent reduction, with a post/pre surgery AUC ratio of 0.47 (± 0.12) at a low therapeutic dose whereas displaying an AUC ratio 0.44 (± 0.13) at a high dose level due to a more extensive reduction in f_a from 0.97 (± 0.07) to 0.45 (± 0.13) (Figure 3.12 and Figure 3.13).



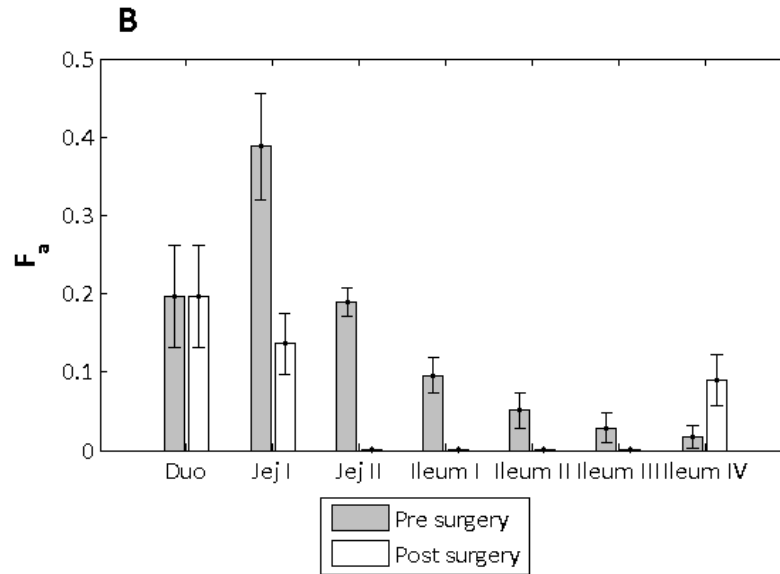


Figure 3.12. Simulated fluconazole immediate release (IR) 400 mg (high therapeutic dose) in morbidly obese (n=100) and post jejunoileal bypass (n=100; small intestinal transit=0.4h) **A:** Mean, 95th and 5th percentile plasma concentration time profile over 24 hours, **B:** Mean and standard deviation of segmental fraction of dose absorbed along the small intestine (f_a). Duo=duodenum, Jej=jejunum.

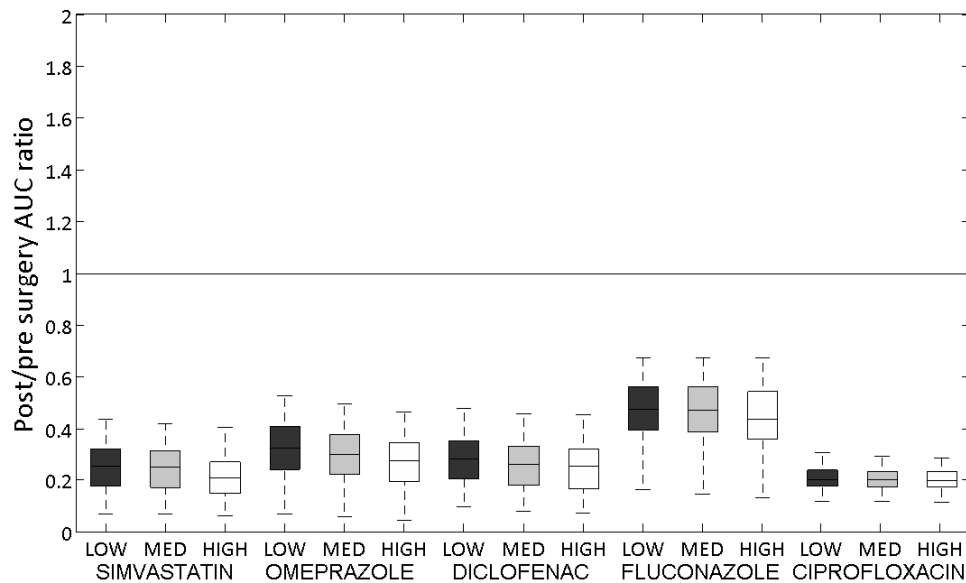


Figure 3.13. Simulated post/pre jejunoileal bypass (small intestinal transit=0.4h) AUC ratio over a range of selected drugs at a low (LOW), medium (MED) and high (HIGH) therapeutic dose: Simvastatin immediate release (IR; 10, 20 and 80 mg), omeprazole enteric coated (EC; 10, 20 and 40 mg), diclofenac EC (25, 50 75 mg), fluconazole IR (50, 200, 400 mg) and ciprofloxacin IR (250, 500 and 750 mg).

Sleeve gastrectomy:

Simulated post sleeve gastrectomy applied to Morbidly Obese did not significantly alter the pre to post surgery drug exposure for the range of studied drugs over low to high therapeutic dose ranges (data not shown).

3.5 Discussion

3.5.1 Simulating oral drug exposure following bariatric surgery:

Simulating oral drug bioavailability following bariatric surgery identified a number of potential pharmacokinetic parameters suggested to influence bioavailability following bariatric surgery.

Simvastatin is characterised as a BCS class IV, and further classified as a BDDCS (Biopharmaceutics Drug Disposition Classification System) class II compound (Darwich *et al.*, 2010; Benet *et al.*, 2011). The drug is considered a low soluble compound at therapeutic dose, displaying an aqueous solubility 0.03 mg/mL (Kasim *et al.*, 2004; BNF, 2011). The drug is administered in its lactone form and undergoes pH and temperature dependent interconversion to its hydroxyacid form at a pH below 6, whereas the lactone form mainly is formed at pH's over the equilibrium (Kearney *et al.*, 1993). Approximately 85% of the administered dose is absorbed, being further exposed to extensive metabolism by CYP3A4 in the small intestine and liver, and CYP3A5 to lesser extent (Lennernas and Fager, 1997; Prueksaritanont *et al.*, 1997).

The simulated increase in drug exposure of simvastatin in the post RYGB (SIT=3.0h) population was due to an increase in F_G post surgery. These findings suggest intestinal gut wall metabolism plays an important role in the observed trend in drug bioavailability pre to post surgery for compounds subject to a high small intestinal metabolic extraction ratio, such as atorvastatin and simvastatin, where simulated post/pre surgical AUC ratio following RYGB was similar to that observed of atorvastatin, displaying a median AUC ratio of 1.20 (0.3-2.3) (Skottheim *et al.*, 2009). Simulated compound characteristics of simvastatin did not incorporate the pH dependent interconversion of the lactone and acid form, but treated this as a part of the CYP3A4 clearance term through fitting to observed data, thus not taking into account

the increased gastric pH following RYGB surgery and its impact on the interconversion (Kearney *et al.*, 1993).

Omeprazole (BCS class II and BDDCS class I ampholyte, $pK_a=8.7$, $pK_b=3.79$), is a sparingly soluble highly lipophilic compound with stability issues at a lower pH levels, thus motivating enteric coated formulation (EC) protecting the drug from degradation caused by the gastric pH (Brandstrom *et al.*, 1985; El-Badry *et al.*, 2009; Darwich *et al.*, 2010; Benet *et al.*, 2011). The drug displays a highly variable absorption and further mainly undergoes hepatic metabolism and clearance by CYP3A4 and 2C19 (Shimamoto *et al.*, 2000). Only a minor alteration in F_G was observed following simulations post BPD-DS, where an increase was observed, overall. The biggest impact was observed on f_a , potentially due to the reduction in absorption area.

Diclofenac (BCS class II; BDDCS class I) is mainly metabolised by CYP2C9 (Shimamoto *et al.*, 2000; Darwich *et al.*, 2010; Benet *et al.*, 2011). The drug undergoes extensive first-pass metabolism, displaying an oral bioavailability of approximately 54% (Willis *et al.*, 1979). Following RYGB and BPD-DS a minor increase in F_G was observed due to the bypass of intestinal regions abundant of CYP2C9, however this was counteracted by a reduction in f_a .

Fluconazole (BCS class I; BDDCS class III) is soluble at a therapeutic dose and displays a bioavailability over 90% in healthy volunteers, further being mainly renally cleared (Brammer *et al.*, 1990; Darwich *et al.*, 2010; Benet *et al.*, 2011). Following bariatric surgery simulated oral drug exposure of fluconazole only displayed minor changes in AUC with the exception following JIB. These results are consistent with observations in AIDS patients, frequently displaying gastrointestinal disturbances, and a case report in a patient subject to gastrointestinal restriction of the gastric antrum, duodenum and ileum following peptic ulcer disease, displaying no altered bioavailability or a comparable bioavailability as compared to healthy volunteers (DeMuria *et al.*, 1993; Joe *et al.*, 1994).

Ciprofloxacin (BCS class III; BDDCS class IV) is sparingly soluble at the therapeutic dose range, further having a reported oral bioavailability ranging from approximately 60 to 80% in healthy volunteers and is mainly renally cleared (Hoffken *et al.*, 1985;

Lettieri *et al.*, 1992; Darwich *et al.*, 2010; Benet *et al.*, 2011). The simulated reduction in AUC following bariatric surgery is therefore most likely an effect of a reduction in absorption area and a product of post-operative solubility issues.

The major issue following SG would be potential solubility issues due to a reduced concomitant fluid volume with the administered dose although this was not a major issue for any of the studied drugs.

3.5.2 Post bariatric surgery ADAM model limitations:

Conclusions drawn from this study are limited by a number of “known unknowns” relating to gastrointestinal physiology post bariatric surgery, where data relating to gastrointestinal pH, small intestinal transit and post surgical gastrointestinal physiological adaptation and whole body physiological alterations, such as hepatic activity and bile secretion and its GI levels, is sparse or nonexistent.

Following RYGB, gastric pH was estimated to increase based on measuring acid secretion in the gastric pouch (mEq/time). Albeit, examining the relationship between pH and gastric acid output the relationship is not straightforward. Pratha, and co-workers (2006), examined the effect of proton pump inhibitors (PPI) on gastric acid output and pH and concluded the relation between pH and gastric acid output to be highly ambiguous. At a gastric acid output of ≤ 1 mEq/30 min a pH 0.9 to 7.7 was observed, whereas a pH of 2.5 and upwards was rendered at minimal gastric acid output, thus rendering a high degree of uncertainty in the implications of mEq/time post Roux-en-Y gastric bypass (Pratha *et al.*, 2006).

Small intestinal transit time estimation following bariatric surgery was limited to one study examining small intestinal transit time of solids in 10 patients subject to total gastrectomy with Roux-en-Y reconstruction (Pellegrini *et al.*, 1986) or estimations based on the extent of small intestinal bypass. As the procedure differs in terms of the extent of gastrectomy as compared to RYGB for the treatment of obesity such an assumption may not necessarily hold true.

Following gastric restrictive surgery, *i.e.* RYGB and SG, gastric emptying of liquid displayed an overall significant reduction, whereas gastric emptying of solids displayed an increase in variability following RYGB. The impact of RYGB surgery on gastric emptying of solids may be due to post surgical state of stasis due to a reduced nervous stimulus (Horowitz *et al.*, 1982; Woodward *et al.*, 1993).

The methodology of how the ADAM model was adapted to mimic post bariatric surgery conditions is subject to a number of limitations due to the limited nature of how the ADAM model could be adjusted through the Simcyp[®] Simulator through the existing interface. Rather than bypassing the proximal small intestinal compartments, the transit time through these compartments were reduced close to zero. As a consequence the modelling and simulations of drug concentration in the bilio limb could not be conducted, thus limiting the predictability of drugs subject to biliary elimination. A further concern was the fluid dynamics within the ADAM model which is governed by secretion and reabsorption of GI fluids taking place throughout the gastrointestinal tract compartments (Valentin, 2002; Jamei *et al.*, 2009b). As a consequence of such parameter alterations not being possible through the Simcyp user-interface an overestimation of GI fluid volumes and consequential underestimation of potential drug specific solubility issues following surgery are possible.

3.6 Conclusions

Trends in pre and post Roux-en-Y gastric bypass bioavailability seem to be highly dependent on drug specific parameters such as affinity to CYP3A4, solubility and permeability issues based on simulated outcome, albeit yet to be confirmed with regards to clinical data. A mechanistic modelling approach has the potential of examining the impact of drug specific parameters on trend of pre to post surgery and to serve as a useful tool in examining the impact of physiological alterations on oral drug bioavailability in the absence of clinical data.

Current limitations in estimating and simulating the impact of oral drug bioavailability following bariatric surgery include the sparsity in clinical data for further model validation and the lack of data on resultant physiological changes post surgery.

3.7 Acknowledgements

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Chapter 4: Evaluation of an *in silico* PBPK post-bariatric surgery model through simulating oral drug bioavailability of atorvastatin and cyclosporine

Chapter 4: Evaluation of an *in silico* PBPK post-bariatric surgery model through simulating oral drug bioavailability of atorvastatin and cyclosporine

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4.1 Abstract

An increasing prevalence of morbid obesity has led to dramatic increases in the number of bariatric surgeries performed. Altered gastrointestinal physiology following surgery can be associated with modified oral drug bioavailability (F_{oral}). In the absence of clinical data, an indication of changes to F_{oral} via systems pharmacology models would be of value in adjusting dose levels after surgery. A previously developed virtual “post-bariatric surgery” population was evaluated through mimicking clinical investigations on cyclosporine and atorvastatin after bariatric surgery. Cyclosporine simulations displayed a reduced fraction absorbed through gut wall (f_a) and F_{oral} after surgery, consistent with reported observations. Simulated atorvastatin F_{oral} post surgery was broadly reflective of observed data with indications of counteracting interplay between reduced f_a and an increased fraction escaping gut wall metabolism (F_G). Inability to fully recover observed atorvastatin exposure after biliopancreatic diversion with duodenal switch highlights the current gap regarding the knowledge of associated biological changes.

4.2 Introduction

The prevalence of obesity has increased dramatically in the USA and Europe over the last decade (Flegal *et al.*, 2010; OECD, 2011). Bariatric surgery has proven to be successful in treating morbid obesity with over 220,000 surgeries performed in the USA and Canada in 2008 (Buchwald and Oien, 2009). Several bariatric surgical methods coexist in healthcare, where Roux-en-Y gastric bypass (RYGB) is considered gold-standard (Picot *et al.*, 2009). RYGB results in a reduced gastric volume, complete bypass of the pylorus, partial bypass of the duodenum and proximal jejunum and a delay in bile inflow to the distal jejunum. The more invasive biliopancreatic diversion

with duodenal switch (BPD-DS) results in a partial resection of the stomach with the pylorus retained, bypass of jejunum and proximal ileum, and an approximate 250 cm delay of the bile inlet. Jejunioileal bypass (JIB) is considered the most invasive procedure, retaining only the stomach (with pylorus) and distal ileum (Darwich *et al.*, 2012a; Darwich *et al.*, 2012b).

As a consequence of bariatric surgery, a number of physiological parameters influencing oral drug bioavailability (F_{oral}) are altered, including: a reduced gastric capacity and emptying time, altered gastrointestinal (GI) pH, reduced absorption area, altered bile flow and small intestinal transit, altered substrate exposure to drug metabolising enzymes and active efflux transporters (Jamei *et al.*, 2009b; Ghobadi *et al.*, 2011; Darwich *et al.*, 2012a). Patients undergoing bariatric surgery continue to receive various therapeutic drugs without dose adjustments for altered bioavailability which can potentially lead to no therapeutic effect or higher than required systemic exposure. There are a very limited number of studies that have investigated oral drug exposure post bariatric surgery (Malone and Alger-Mayer, 2005; Darwich *et al.*, 2012a).

The direction and magnitude of impact on F_{oral} following surgery may depend on the characteristics and invasiveness of the surgical procedure, where the extent of the small intestinal bypass may influence the fraction of dose absorbed through the gut wall (f_a) (Skottheim *et al.*, 2009; Skottheim *et al.*, 2010). Bypassing regions highly abundant in drug metabolising enzymes can affect the fraction of absorbed drug escaping gut wall metabolism (F_G) (Darwich *et al.*, 2012b). F_H , the fraction that escapes hepatic first-pass metabolism, may be assumed to remain unaltered (Equation 1.1) (Jamei *et al.*, 2009b; Ghobadi *et al.*, 2011; Darwich *et al.*, 2012a).

$$F_{oral} = f_a \cdot F_G \cdot F_H$$

Equation 1.1: Components of F_{oral} .

A level of uncertainty remains regarding the small intestinal transit (SIT) post surgery where a reduction in motility has been observed, albeit well powered clinical studies of small intestinal transit in man are lacking (Pellegrini *et al.*, 1986; Suzuki *et al.*, 2005; Darwich *et al.*, 2012b).

The post surgical physiology is further complicated by the possibility of small intestinal trauma or adaptation, where an enhanced permeability due to impairment of the mucosa or long-term villi elongation has been observed in rat BPD-DS models (Gaggiotti *et al.*, 1995; Mendieta-Zeron *et al.*, 2011). Alterations in levels of gastric hormones (including: peptide YY, ghrelin and Glucagon-Like Peptide 1) may lead to redistribution of intestinal blood flow to the submucosa, as observed in dog models. Post surgical hormonal levels have been observed to vary depending on the bariatric surgical procedure (Savage *et al.*, 1987; Buell and Harding, 1989; Suzuki *et al.*, 2005; Garcia-Fuentes *et al.*, 2008).

Due to these multi-factorial changes, physiologically-based pharmacokinetic (PBPK) modelling enables one to predict *in silico*, the effects of various bariatric surgeries in a morbidly obese population (Darwich *et al.*, 2012b). The Advanced Dissolution Absorption and Metabolism (ADAM) model describes the variability in F_{oral} through a physiologically-based seven segment model of the small intestine, including: duodenum, jejunum I and II, and ileum I-IV. The model describes drug release from formulation, dissolution, precipitation, degradation, absorption, active transport and metabolism as the drug transits through the small intestine, allowing the incorporation of saturation effects and population variability. The ADAM model has been well described and utilised in previous literature (Jamei *et al.*, 2009b).

In our previous work, a virtual ‘post bariatric surgery’ population was created utilising the ADAM model within a PBPK system containing characteristics of a morbidly obese population. Developed models for RYGB, BPD-DS and JIB included specific anatomical and physiological parameters that are altered following surgery, namely: Gastric capacity and fluid dynamics, gastric emptying time, small intestinal bypass, GI pH, bile flow and alterations to regional abundance of drug metabolising enzymes (*e.g.* CYP3A) and efflux transporter P-glycoprotein. The model further incorporated whole body physiological changes, such as post surgical recovery of renal function as a function of weight loss (Darwich *et al.*, 2012b).

Simulations predicted change in oral bioavailability of various drugs pre to post bariatric surgery revealing the magnitude and direction of the effect to be surgery dependent, due to altered GI system parameters, and influenced by a complex interplay between drug characteristics, including: solubility, permeability, dissolution, gut wall metabolism and dose level. However, no comparison so far has been made between the results of these simulations and existing clinical data (Darwich *et al.*, 2012b).

In the current study, we report on the evaluation of previously developed post bariatric surgery models by comparing the observed versus predicted impact of bariatric surgery on oral exposure of cyclosporine and atorvastatin acid using virtual simulations.

4.3 Methods

4.3.1 Bariatric surgery model

Sex, age, height and weight matched simulations were carried out corresponding to identified clinical studies (Marterre *et al.*, 1996; Chenhsu *et al.*, 2003; Skottheim *et al.*, 2009; Skottheim *et al.*, 2010) utilising the ADAM model coupled to a full PBPK distribution model, incorporated into the Simcyp[®] Simulator (Simcyp Ltd., Sheffield, UK) (Equation 4.1, Equation 4.2 and Equation 4.3) (Jamei *et al.*, 2009a; Jamei *et al.*, 2009b). Detailed specification for the demographics and physiological parameters of the morbidly obese population have been published previously. Similarly, surgical changes to the anatomy and physiology of gastrointestinal tract following bariatric surgeries, including: RYGB, BPD-DS and JIB, are defined in an earlier publication. Study population specific surgical alterations are summarised in (Table 4.1).

$$Height = C0 + C1 \cdot Age + C2 \cdot Age^2$$

Equation 4.1: Height equation.

$$Weight = e^{(C0 + C1 \cdot Height)}$$

Equation 4.2: Weight equation.

$$BSA = Weight^{Weight\ exponent} \cdot Height^{Height\ exponent}$$

Equation 4.3: Body surface area equation.

Table 4.1. Summary of alterations to population template in order to mimic and simulate post surgical conditions.

Parameters	Bariatric surgical procedures			References
	JIB	RYGB	BPD-DS	
Gastric emptying: Liquids (minutes)	24 ^A CV: 38%	7 CV: 45%	24 ^A CV: 38%	(Horowitz <i>et al.</i> , 1982; Hedberg <i>et al.</i> , 2011a; Darwich <i>et al.</i> , 2012b)
Gastric capacity (mL)	250 ^A	30	150	(Wittgrove and Clark, 2000; Darwich <i>et al.</i> , 2012b)
Q _{sec} stomach (L/h)	0.108	0.059	0.295	
Initial volume of stomach fluid (mL)	50 ^A	9.9	32.6	
Gastric pH	1.5 ^A	6.5	1.5 ^A	(Smith <i>et al.</i> , 1993; Behrns <i>et al.</i> , 1994; Hedberg <i>et al.</i> , 2011b; Darwich <i>et al.</i> , 2012b)
Small intestinal bypass (centimeters and/or segments)	Retaining the duodenum, 20% of jejunum I and 23% of ileum IV. ^B	100 cm (duodenum and jejunum I) ^B	Retaining 2.5 cm of duodenum and 250 cm of the distal ileum ^C	(Wittgrove and Clark, 2000; Darwich <i>et al.</i> , 2012b)
Bile exclusion (centimeters and segments)	Not applicable (jej II – ileum III)	110 cm (stomach – jejunum I)	252 cm (stomach – ileum III)	
CYP3A4 abundance (nmol/total gut)	32.3 CV: 60%	48.3 CV: 60%	12.6 ^D CV: 38%	
CYP3A5 abundance (mmol/total gut)	12.1 CV: 60%	18.0 CV: 60%	10.1 ^D CV: 38%	
Mean small intestinal transit time (hours) – Scenario 1	0.4 $\alpha = 0.5$ $\beta = 0.4$	3.0 $\alpha = 2.6$ $\beta = 3.7$	1.2 $\alpha = 1.3$ $\beta = 1.9$	
Mean small intestinal transit time (hours) – Scenario 2	0.7 $\alpha = 0.6$ $\beta = 0.4$	5.0 $\alpha = 4.0$ $\beta = 5.3$	4.2 ^E $\alpha = 3.7$ $\beta = 5.0$	(Pellegrini <i>et al.</i> , 1986; Savage <i>et al.</i> , 1987; Suzuki <i>et al.</i> , 2005; Darwich <i>et al.</i> , 2012b)
Renal equation	MDRD	MDRD	MDRD	{Chagnac, 2003 #78; Darwich, 2012 #521; Navarro-Diaz, 2006 #79; Saliba, 2010 #76; Serra, 2006 #80 (6, 37-40)}

JIB=Jejunioleal bypass, RYGB=Roux-en-Y gastric bypass, BPD-DS=Biliopancreatic diversion with duodenal switch. Q_{sec}=Secretion flow.

^AUnaltered parameter as compared to morbidly obese controls.

^BSetting human effective permeability (P_{eff}) of compounds close to zero in bypassed segments.

^CAltering small intestinal parameters in the ADAM model to conform to remaining segments.

^DBased on intestinal biopsy in the study population (11).

^EDerived based on a pre to post surgical peptide YY level of 413% utilising linear relation between peptide YY and small intestinal transit time as reported by Savage, and co-workers (16, 18).

α & β = Weibull scaling factors utilising assuming a variance of 1.8h.

MDRD=Modification of Diet Renal Disease equation.

Cyclosporine

The cyclosporine compound file, available in the Simcyp[®] Simulator compound library, was adapted to account for formulation properties corresponding to Sandimmune[®] solution and Sandimmune[®] Neoral[®] microemulsion (Novartis), using an aqueous solubility of 0.01 mg/mL and particle sizes of 3.73 μm and 0.03 μm respectively, further allowing Neoral[®] to supersaturate freely without precipitation assuming a linear dose-concentration relationship (Mueller *et al.*, 1994). A full PBPK model was utilised to describe the cyclosporine distribution, where tissue to plasma partition coefficients (Kp's) were obtained from tissue to plasma concentrations at steady state following intravenous infusion were obtained from rat (Bernareggi and Rowland, 1991).

Atorvastatin acid

Physicochemical parameters for atorvastatin acid were taken from the publication by Lennernas (Lennernas, 2003). Metabolic data were obtained from the *in vitro* study reported by Jacobsen, and co-workers (Jacobsen *et al.*, 2000); CYP3A4 was found to be the main enzyme involved in the formation of the two primary metabolites ortho- and para-hydroxyatorvastatin acid with a minor contribution from CYP2C8. Intersystem extrapolation factors (ISEFs), which correct for differences in intrinsic activity per unit CYP enzyme relative to its native environment were applied to the kinetic data for recombinantly expressed CYP3A4 and CYP2C8, respectively. Acyl glucuronidation of atorvastatin acid to the lactone and UDPGA-dependent metabolism of atorvastatin acid mainly via UGT1A1 to a minor ether glucuronide was also considered (Prueksaritanont *et al.*, 2002; Goosen *et al.*, 2007). The resultant intrinsic clearance data were scaled to whole organ values according to Equation 4.4 and Equation 4.5 (Howgate *et al.*, 2006). The uptake of atorvastatin acid has been demonstrated in an OATP1B1-transfected cell system (HEK293 cells) (Lau *et al.*, 2007; Amundsen *et al.*, 2010). While these *in vitro* data support the involvement of OATP1B1 in the hepatic uptake of atorvastatin acid, it was found that when used in combination with the metabolic data, the clearance was significantly under-predicted. In order to recover the plasma concentration time profile of atorvastatin acid prior to BPD-DS, $J_{\text{max,OATP1B1}}$ and $K_{\text{p,muscle}}$ were re-estimated to 532.4 pmol/min/million cells and 4.0, utilising weighted least square Nelder-Mead minimisation method in the parameter estimation toolbox within the Simcyp[®] Simulator (Skottheim *et al.*, 2010).

$$CLu_{H,int} = \frac{ISEF \cdot V_{\max-rhCYP} \cdot Abundance \cdot MPPGL \cdot LiverWeight}{K_{m,u}}$$

Equation 4.4: IVIVE of $CLu_{H,int}$ from rCYP.

$$CLu_{G,int} = \frac{ISEF \cdot V_{\max-rhCYP} \cdot Abundance}{K_{m,u}}$$

Equation 4.5: IVIVE of $CLu_{G,int}$ from rCYP.

Sensitivity analysis was carried out with regards to potential gastrointestinal physiological parameters subject to potential alterations following surgery due to hormonal alterations, including: small intestinal transit time, villous blood flow (Q_{villi}), gastric emptying, small intestinal bile concentration, the enterocyte volume in the remaining small intestine (V_{ent}), post-surgical abundance of gastrointestinal CYP3A (GI CYP3A) and small intestinal effective permeability (P_{eff}).

Analysis

Simulated data was visually inspected against observed data. In addition, the potential mechanism of changes to oral drug absorption was examined through the simulations in terms of assessing the effects on plasma drug concentration time profile, maximum plasma drug concentration (C_{\max}), time of maximum plasma drug concentration (t_{\max}), f_a and F_G .

4.4 Results

Changes in oral drug bioavailability post bariatric surgery were demonstrated for cyclosporine and atorvastatin acid following Roux-en-Y gastric bypass (RYGB), biliopancreatic diversion with duodenal switch (BPD-DS) and jejunoileal bypass (JIB) (Marterre *et al.*, 1996; Chenhsu *et al.*, 2003; Skottheim *et al.*, 2009; Skottheim *et al.*, 2010). Sex, age, height and weight matched simulations were carried out based on corresponding clinical studies utilising post bariatric surgery models coupled to a full

PBPK distribution model into the Simcyp[®] Simulator. The results from the comparison of observed versus simulation studies are as follows:

4.4.1 Cyclosporine

Roux-en-Y gastric bypass

Following RYGB, Marterre and co-workers (Marterre *et al.*, 1996) reported a 194% increase in the daily dose per kg body weight in kidney transplant patients (n=3) of cyclosporine A (CsA) Sandimmune[®] solution. CsA trough blood levels were monitored from 6 months prior to RYGB up to 12 months postoperatively, using a TDx immunoassay. The observed reduction in exposure prompted an increase in the oral dose from 1.8 (± 0.5) to 3.5 (± 1.1) mg/kg/day in order to maintain pre-RYGB CsA trough levels (Figure 8.1 A-D) (Marterre *et al.*, 1996). Due to the reported over prediction of the TDx immunoassay, observed and simulated data were normalised for trough levels immediately before RYGB surgery, indicated by the time of 0 months (Figure 8.1 B and C) (Steimer, 1999).

In an age, sex, and weight matched virtual population, oral drug exposure of Sandimmune[®] CsA solution was simulated in 10 randomised trials consisting of 3 individuals in each trial (n=10·3). Cyclosporine displayed a reduction in f_a from 0.40 (5-95% confidence interval [CI95]: 0.24-0.59) to 0.19 (0.10-0.32) following RYGB, at a simulated small intestinal transit (SIT) time of 3.0h; whereas F_G remained unaltered at 0.86 (0.74-0.87). A 194% increase in dose level, resulted in a trough level ratio of 0.96 (0.58-1.44) as compared to the pre operative exposure at 0 months. Assuming a post surgical small intestinal transit time of 5.0h, cyclosporine displayed reduction in f_a to 0.26 (0.14-0.41), F_G remained unaltered. A 194% increase in the dose level resulted in an over prediction in post RYGB CsA trough levels, with a simulated post/pre surgical ratio of 1.45 (0.85-2.19) as compared to pre operative exposure at 0 months (Figure 8.1 A-D).

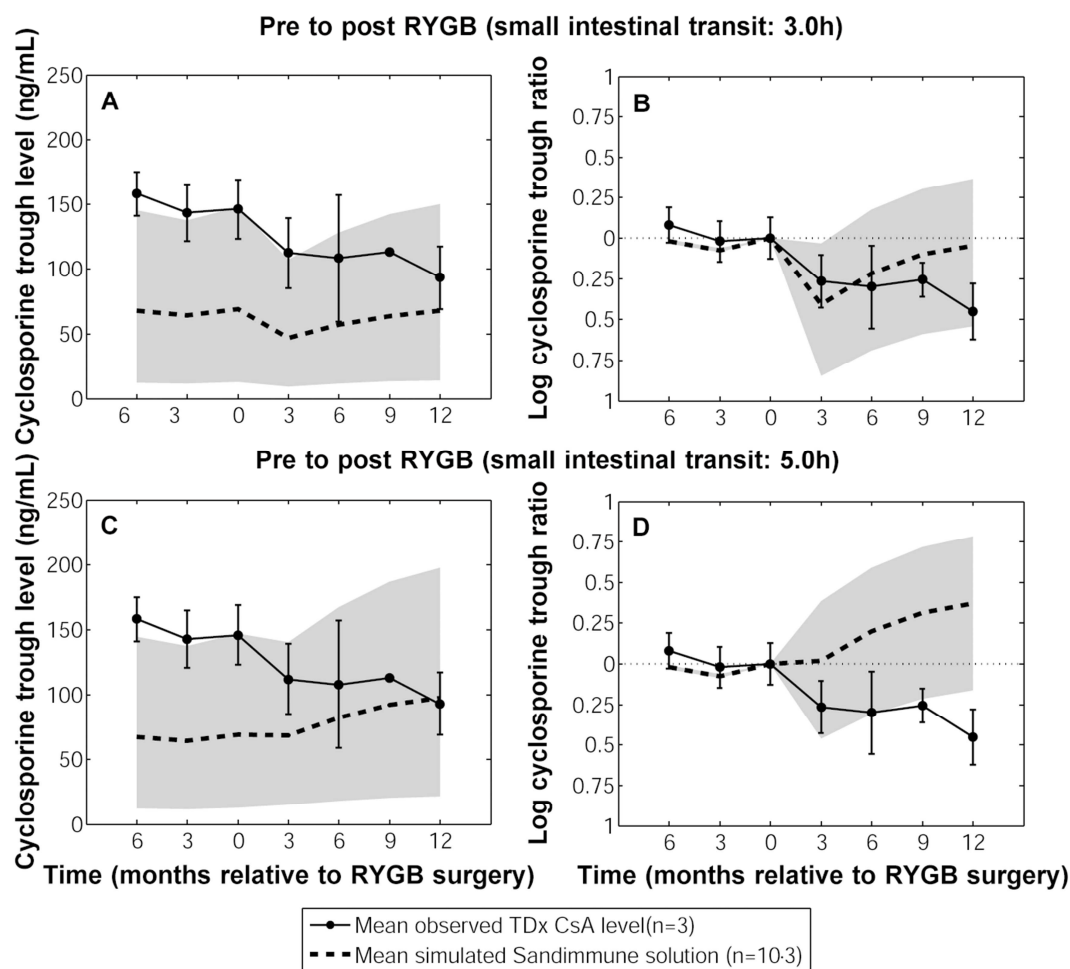


Figure 4.1. Mean and standard deviation of observed cyclosporine (CsA) TDx trough levels at steady state pre to post Roux-en-Y gastric bypass (RYGB) at -6, -3, 0, 3, 6, 9 and 12 months relative to RYGB surgical event (0 months). Time points from -6 to 12 months correspond to dose levels of: 1.7, 1.7, 1.8, 2.4, 2.8, 3.2, 3.5 mg/kg/day respectively (n patients=3) administered twice daily. Observed data is compared to simulated 50, 95 and 5% prediction interval, indicated by grey area, of cyclosporine Sandimmune[®] trough levels (n patients=10·3), A: Simulated post RYGB at a small intestinal transit time (SIT) of 3.0h, B: Log normalised simulated CsA trough ratio as compared to 0 months (RYGB SIT=3.0h), C: Simulated CsA trough levels at RYGB SIT of 5.0h, D: Log normalised simulated CsA trough ratio as compared to 0 months (RYGB SIT=5.0h) (Marterre *et al.*, 1996).

Simulations of the theoretical impact of RYGB on the solubilisation enhanced cyclosporine Neoral[®] microemulsion, at a post surgical SIT of 3.0h, produced an AUC ratio of 1.84 (1.26-2.37) at 12 months post surgery as compared to levels at 0 months

relative to RYGB surgery. The observed increase in oral exposure of Neoral[®] was due to a 194% dose increase, where f_a displayed an increase from 0.72 (0.47-0.92) to 0.82 (0.57-0.94); whereas F_G increased from 0.90 (0.81-0.96) to 0.94 (0.90-0.98) (Appendices 8.3).

Jejunioileal bypass

In a case study by Chenhsu, and co-workers (2003), CsA blood levels at 2 hours post administration at steady state (C2) administered as Neoral[®] microemulsion in controls (n=7) and post JIB (n=1), displayed a reduced exposure when comparing the mean C2 concentration over the administered dose range, reporting a reduction in C2 levels of approximately 59% (Chenhsu *et al.*, 2003).

Simulating demographically matched morbidly obese controls (n=10·7) and post JIB patients (SIT=0.4h; n=10·1), cyclosporine displayed a reduction in C2 levels from 452 (153-776) to 357 (103-650) ng/mL at a dose level of 4 mg/kg/day and from 2,528 (388-6089) to 1,632 (571-2,811) ng/mL, at a dose of 12 mg/kg/day. Simulated levels corresponded well with the linear regression of observed data as compare to the 5-95% prediction interval. The simulated reduction in oral drug exposure in the post JIB population as compared to controls was due to a reduction in f_a from 0.61 (0.35-0.86) to 0.12 (0.04-0.19); whereas F_G displayed a minor reduction from 0.90 (0.79-97) to 0.88 (0.75-0.96) at a therapeutic dose of 2 mg/kg/day. At a dose of 12 mg/kg/day a major reduction in f_a was observed from 0.34 (0.16-0.53) to 0.08 (0.01-0.18) whereas F_G was reduced from 0.91 (0.81-0.93) to 0.90 (0.80-0.97) (Figure 4.2).

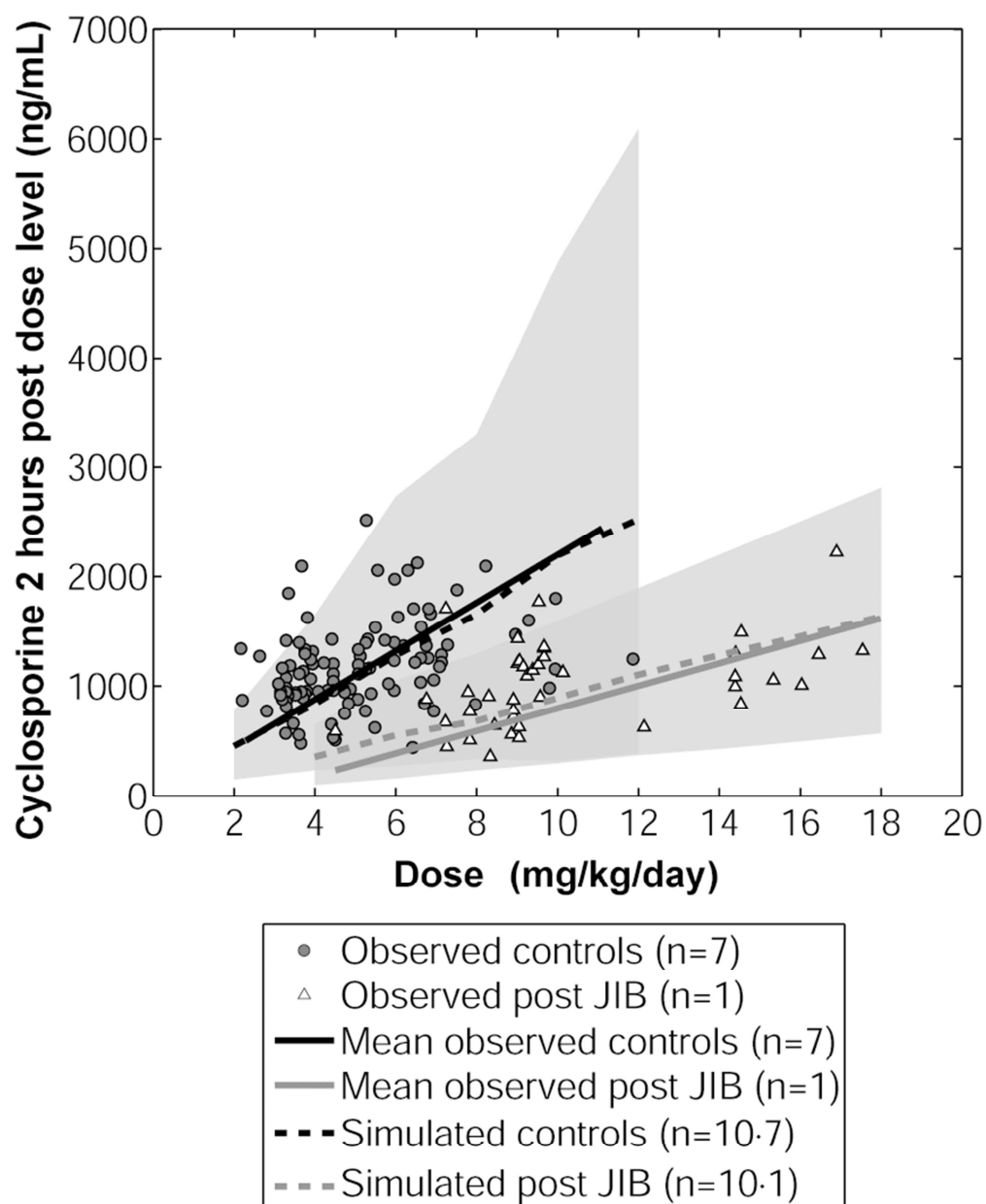


Figure 4.2. Observed mean blood concentration of cyclosporine microemulsion (Sandimmune® Neoral®, Novartis) at steady state 2 hours post dosing in controls (n =7) and one patient (n=1) post jejunoileal bypass (JIB) as compared to simulated sex and age matched controls (n=300) and post JIB (n patients=800) at a small intestinal transit time of 0.4 hours over dose range of 300 to 1,000 mg, where 5, 50 and 95% prediction intervals are indicated by grey areas (Chenhsu *et al.*, 2003).

Assuming a SIT of 0.7h post JIB, cyclosporine displayed a less apparent reduction in C₂ levels due to a less apparent reduction in f_a to 0.19 (0.05-0.30) and 0.13 (0.02-0.26)

at corresponding dose levels of 2 and 12 mg/kg/day respectively. Post JIB (SIT=0.7h), F_G was altered to 0.89 (0.79-0.96) and 0.92 (0.84-0.98) at a therapeutic dose level of 2 and 12 mg/kg/day respectively (Appendices 8.3).

4.4.2 Atorvastatin

Roux-en-Y gastric bypass

In a clinical trial carried out on 12 morbidly obese patients, atorvastatin was administered as an immediate release (IR) tablet of 20-80 mg in fasted state where patients were allowed to eat two hours post administration. Plasma concentration profiles were obtained from 0-8 hours after drug administration pre and three to six weeks post RYGB. The pre to post surgical trend in oral exposure displayed a high variability where the overall reported trend displayed a median post/pre surgery AUC ratio of 1.12 (range: 0.34-2.33), albeit being statistically insignificant (Skottheim *et al.*, 2009).

Virtual simulations for oral drug exposure of atorvastatin acid pre to post RYGB were conducted in 10 randomised trials, each consisting of 12 age, sex and BMI matched individuals (n=10-12). Assuming a reduction in small intestinal transit as function of the small intestinal bypass (SIT=3.0h), resulted in an overall increase in AUC with a simulated median post/pre surgical AUC ratio of 1.13, capturing 100% of observed data within the simulated 95% prediction interval of 0.27-3.80 (Figure 4.3). Alternatively, with an increase in small intestinal transit time post RYGB (SIT=5.0h), atorvastatin acid displayed a median post/pre surgical AUC ratio of 1.42 (0.34-4.91) (Appendices 8.3).

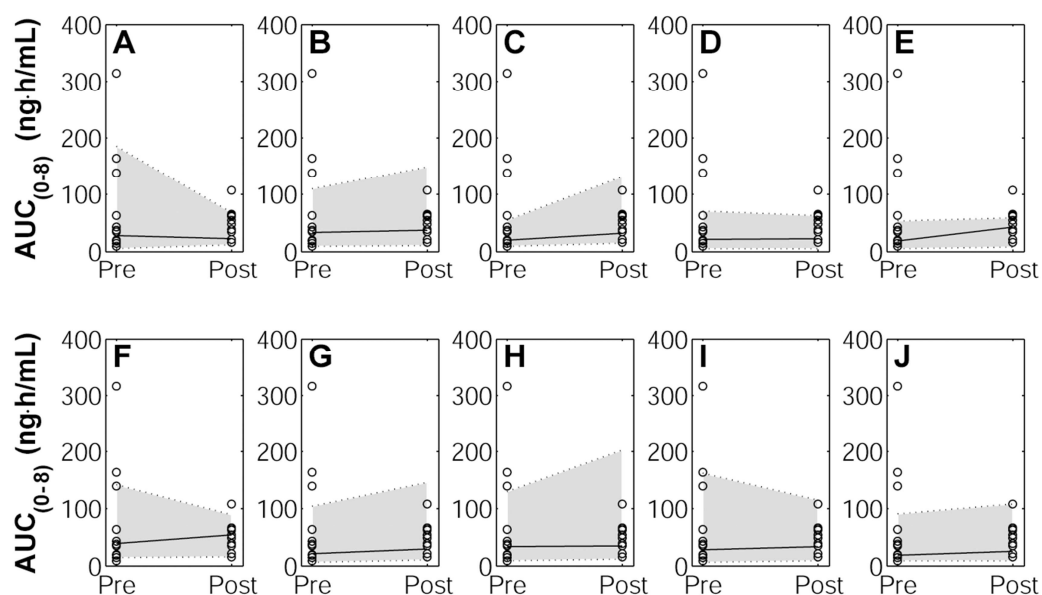


Figure 4.3. Simulated 50, 95 and 5% prediction interval (indicated by grey areas) of oral drug exposure of atorvastatin acid in randomised trials of age, sex, dose and BMI (Body Mass Index) matched patients pre to post Roux-en-Y gastric bypass surgery (small intestinal transit=3.0h) as compared to observed data A-J: Ten randomised simulated trials consisting of 10 individuals in each trial (n individuals=10·12), as compared to observed (n =12; \circ) (Skottheim *et al.*, 2009).

Simulated increase in exposure of atorvastatin following RYGB (SIT=3.0h) was due to a reduction in f_a from 0.58 (0.33-0.77) to 0.54 (0.29-0.74) counteracted by an increase in F_G from 0.69 (0.48-0.86) to 0.73 (0.53-0.88) (Figure 4.4). Assuming a reduced small intestinal motility (RYGB SIT=5.0h), the more apparent increase in AUC was the result of an extensive increase in f_a .

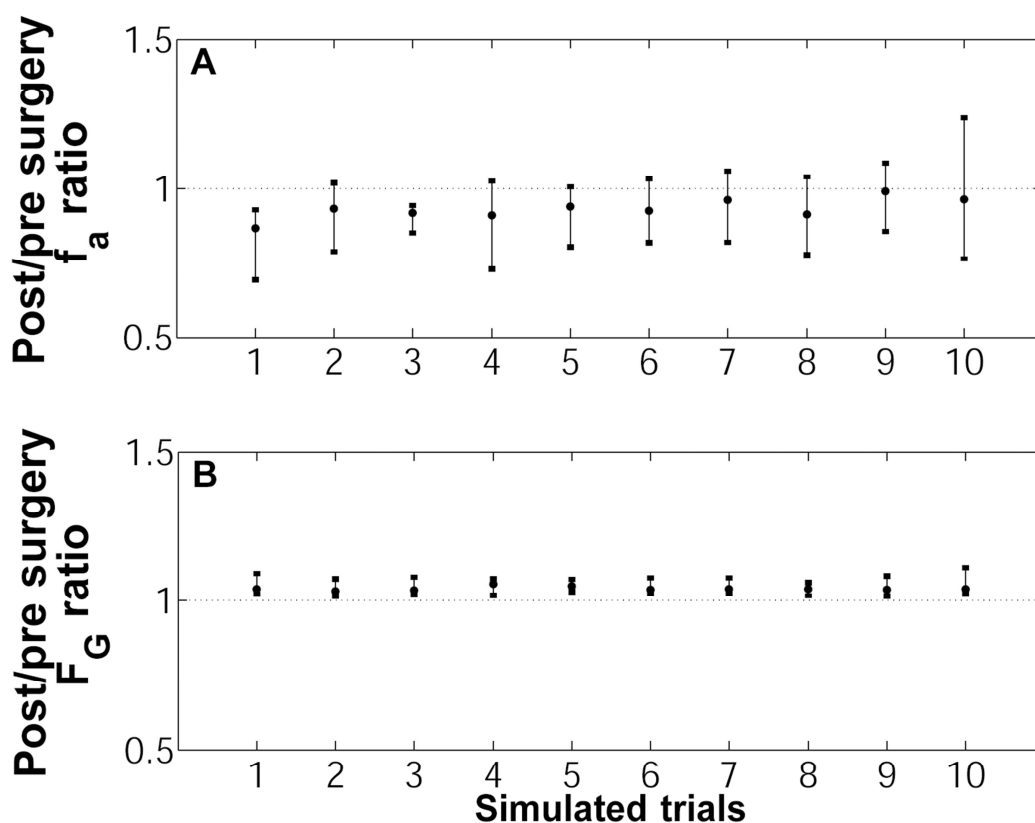


Figure 4.4. Simulated 50, 95% and 5% prediction intervals of the ratio of A: fraction of dose absorbed in the intestine (f_a), and B: fraction escaping gut wall metabolism (F_G) of atorvastatin acid pre to post Roux-en-Y gastric bypass surgery (small intestinal transit=3.0h) in ten individually simulated randomised trials (1-10) consisting of ten individuals in each pre and post surgery (n individuals=10·10) (Skottheim *et al.*, 2009).

Biliopancreatic diversion with duodenal switch

Atorvastatin IR tablet 20-80 mg administered in the fasted state, allowing feeding at 2 hours, displayed a significant increase in oral drug exposure following BPD-DS in 10 morbidly obese patients, with an observed mean AUC ratio of 2.0 (± 1.0) and observed increase in the C_{max} from 20.0 ng/mL (± 24.9) to 28.0 (± 22.5), whereas t_{max} increased from 1.2h (± 0.8) to 2.3h (± 1.0) post BPD-DS (Skottheim *et al.*, 2010).

Predicted plasma concentration-time profiles of atorvastatin acid were consistent with observed data prior to surgery in a morbidly obese population (Appendices 8.3).

However, simulated plasma concentration-time profiles following BPD-DS (SIT=1.2h) were unable to capture the observed increase in oral drug exposure. The predicted AUC ratio of 0.90 (0.16-2.24), was lower than expected due to a reduction in f_a from 0.61 (0.34-0.79) to 0.39 (0.06-0.72) which was counteracted by an increase in F_G from 0.69 (0.59-0.79) to 0.72 (0.63-0.81). C_{max} displayed a minor increase, with a post/pre BPD-DS C_{max} ratio of 1.32 (0.31-2.38), whereas t_{max} displayed a post/pre BPD-DS ratio of 0.62 (0.31-1.00). The simulated pre to post BPD-DS alterations in AUC, C_{max} and t_{max} correspond to the central points of Figure 4.5A, B and C respectively.

Sensitivity analysis was performed to assess the impact of potential physiological alterations post surgery on the plasma exposure of atorvastatin acid, including the impact of: SIT, gastric emptying time, bile concentration in the terminal ileum, small intestinal enterocyte volume (V_{ent}), gastrointestinal CYP3A content (GI CYP3A) and small intestinal permeability (P_{eff}). The AUC was insensitive to changes in the post surgical bile concentration and V_{ent} . Following BPD-DS (SIT=1.2h) a five-fold increase in P_{eff} led to a post/pre surgical AUC ratio of 1.93 (0.60-5.53), whereas C_{max} displayed a post/pre surgical ratio of 4.36 (1.23-9.68). A five-fold increase in Q_{villi} resulted in a minor increase in AUC with a simulated post/pre AUC BPD-DS ratio of 1.24 (0.22-3.24) and a C_{max} ratio of 1.86 (0.47-4.19). A reduction in GI CYP3A by 5-fold, gave a post/pre BPD-DS AUC ratio of 1.13 (0.19-3.06) (Figure 4.5).

Pre to post BPD-DS (SIT=4.2h) displayed an AUC ratio of 1.71 (0.74-5.79), C_{max} ratio of 1.56 (0.69-3.39) and a t_{max} ratio of 0.87 (0.51-1.31). In the sensitivity analysis a two-fold increase in Q_{villi} resulted in a post/pre surgery AUC ratio of 2.07 (0.86-6.96) and a C_{max} ratio of 1.91 (0.84-4.22), whereas t_{max} remained unaltered. A two-fold increase in P_{eff} displayed a post/pre BPD-DS AUC ratio of 2.11 (0.90-6.91), a C_{max} ratio of 2.64 (1.17-5.66) and a minor reduction in t_{max} . A two-fold reduction in GI CYP3A gave a post/pre surgery AUC ratio of 1.99 (0.83-6.76), whereas C_{max} saw a minor increase, displaying an AUC ratio of 1.80 (0.79-4.00). Gastric emptying had the most apparent impact on t_{max} , where a five-fold increase resulted in a post/pre BPD-DS ratio of 1.78 (1.11-2.58) (Figure 4.5).

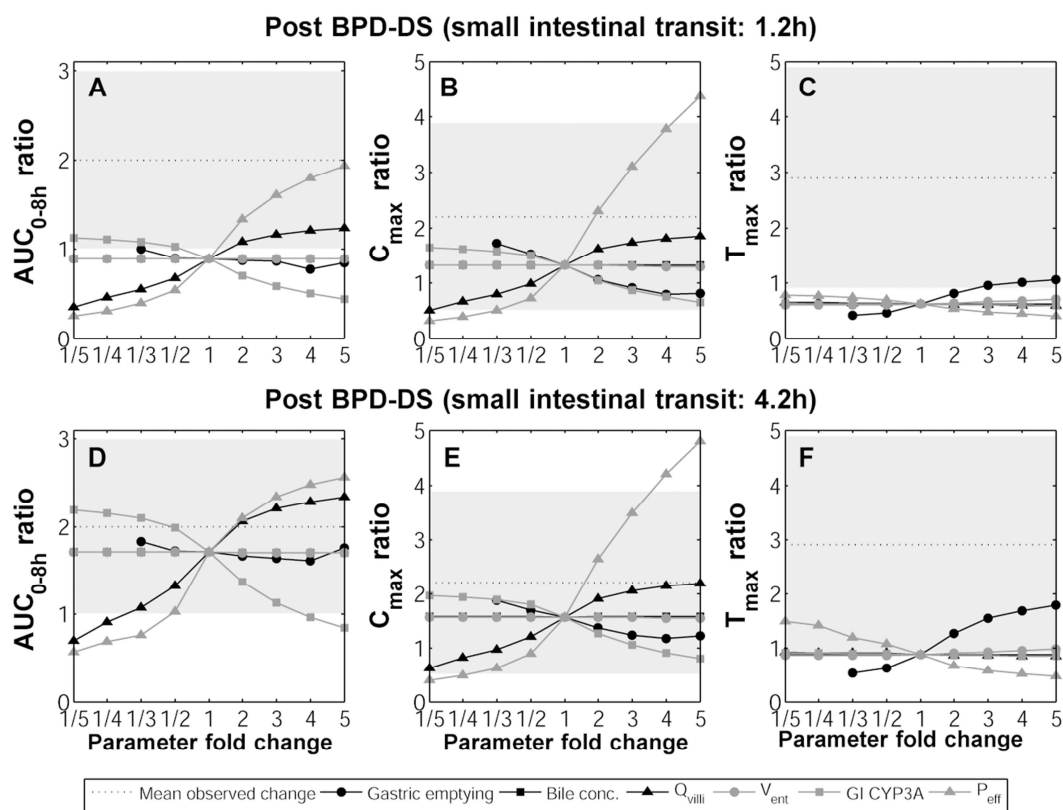


Figure 4.5. Spider plot of sensitivity analysis of simulated post/pre biliopancreatic diversion with duodenal switch (BPD-DS) at a small intestinal transit time (SIT) of 1.2h A: AUC_{0-8h} , B: C_{max} and C: t_{max} ratio, BPD-DS (SIT=4.2h) D: AUC_{0-8h} , E: C_{max} and F: t_{max} ratio, examining the impact of the fold change in physiological parameters: gastric emptying, ileal bile concentration (bile conc.), villous blood flow (Q_{villi}), enterocytic volume (V_{ent}) in the remaining post surgical small intestine, post BPD-DS gastrointestinal CYP3A content, small intestinal permeability (P_{eff}), as compared to mean observed ratio pre to post BPD-DS.

4.5 Discussion

4.5.1 Cyclosporine

The immunosuppressant cyclosporine (molecular weight 1202.61 g/mol) displays poor aqueous solubility and a relatively low permeability due to its lipophilic and bulky character making the compound dependent on bile mediated solubility to facilitate absorption (Venkataramanan *et al.*, 1985; Mehta *et al.*, 1988). The drug is mainly metabolised by CYP3A4 in the intestine and liver and is subject to P-glycoprotein

efflux (Lown *et al.*, 1997; Wojcikowski *et al.*, 2003). The oral bioavailability displays a high interindividual variability, ranging from 5-89% for Sandimmune[®] formulation, whereas Neoral[®] displays improved absorption properties and an oral bioavailability of 21-73% (Paine *et al.*, 2000).

The simulated underprediction of Sandimmune[®] TDx trough levels prior to RYGB surgery was expected and is most likely due to the unspecificity of the immunoassay displaying a high cross-reactivity between the parent compound and metabolites resulting in a significantly higher variability in the trough levels as compared to peak concentrations (Marterre *et al.*, 1996; Steimer, 1999).

Normalising simulated cyclosporine trough levels to pre RYGB levels produced a reduction in exposure comparable to observed data. Further, a simulated 194% increase in Sandimmune[®] dose levels recovered pre surgical trough levels as stated in the publication (Marterre *et al.*, 1996).

In the simulation study of cyclosporine Neoral[®] microemulsion pre to post JIB, observed data of the control population was well described within the 95% prediction interval of the simulated data; whereas the observed exposure post JIB was well described within the 95% prediction interval of simulated data assuming a reduction in small intestinal transit time equivalent to the bypass (SIT=0.4h). An alternative ‘what-if’ scenario simulating a longer transit time (SIT=0.7h) over predicted the observed mean blood concentration post JIB as reported by Chenhsu, and co-workers (Figure 4.2). The overprediction could suggest small intestinal motility to remain unaltered following JIB or be a result of a small post surgical study population (n=1), displaying a low study power, albeit the simulated magnitude of reduction in C2 levels post JIB (SIT=0.4h) closely matched the estimated reduction in cyclosporine exposure following JIB in another case study where a patient was subject to a surgical reversal of the procedure. The reversed JIB produced an observed 2.78-fold increase in exposure in the case study (Knight *et al.*, 1988; Chenhsu *et al.*, 2003).

The simulated discrepancy in oral drug exposure of Sandimmune[®] and Neoral[®] pre to post RYGB, where bariatric surgery had the highest effect on the oral bioavailability of Sandimmune[®], highlights the importance of formulation characteristics and its impact

on oral drug bioavailability pre to post bariatric surgery. The choice of a solubilised biopharmaceutical formulation such as a self-micro-emulsifying drug delivery system, solution or dispersible tablet may be considered as a first hand choice for patients undergoing bariatric surgery and are treated with limited solubility drugs with a narrow therapeutic index. This suggestion supports earlier observations in clinical practice, where alterations in pharmacotherapy post bariatric surgery aim at switching to formulations displaying improved dissolution properties (Darwich *et al.*, 2012a).

Atorvastatin

The HMG-CoA reductase inhibitor atorvastatin, which is administered in the acid form, displays a high solubility and permeability. The compound is extensively metabolised in the small intestine and liver, namely by CYP3A4 but also via the UGT1A1 and UGT1A3 route. Atorvastatin acid and the lactone metabolite are also subject to inter-conversion by the UGTs and another minor chemical pathway. Atorvastatin acid is a substrate of P-glycoprotein efflux and OATP1B1 mediated active hepatic uptake (Lennernas, 2003).

Trends in simulated oral drug exposure of atorvastatin pre to post RYGB were consistent with observed data, where simulated trends in f_a and F_G suggested that an interplay between reduced absorption area and bypass of regions highly abundant in CYP3A is of high importance when considering the overall effect on oral bioavailability. Simulated RYGB (SIT=3.0h) produced the closest agreement with observed data of atorvastatin exposure following RYGB, again suggesting a reduction in small intestinal transit time to be the most likely consequence of surgery (Skottheim *et al.*, 2009).

The inability to recover the observed 2-fold increase in atorvastatin AUC pre to post BPD-DS at a simulated SIT of 1.2h, may suggest additional post surgical physiological parameters to be governing the trend in oral drug bioavailability post BPD-DS. The exploratory sensitivity analysis identified a number of potential parameters leading to a comparable increase in oral drug exposure pre to post BPD-DS. An increase in small intestinal transit following BPD-DS, corresponding to the linear regression relationship between mouth to caecum transit time and plasma levels of peptide YY, resulted in an AUC ratio of 1.71 (0.74-5.79). Further, a simulated two-fold increase in P_{eff} and Q_{villi} , or

a two-fold reduction in the gastrointestinal content of CYP3A post BPD-DS (SIT=4.2h) recovered the observed AUC of atorvastatin. The reoccurring under prediction of t_{\max} following surgery may be explained by an altered postprandial response causing a delayed absorption.

These findings suggest that additional physiological parameters, such as impairment in permeability or redistribution of intestinal blood flow, may play an important role in governing trends in oral drug exposure pre to immediately post BPD-DS. The results highlight the surgery specific trends observed post bariatric surgery due to the intricate interplay between fluid dynamics, absorption area, transporters, metabolism and gastrointestinal physiology.

Current limitations in simulating the impact of oral drug bioavailability following bariatric surgery include the lack of clinical and post surgical physiological data. Nonetheless, the models integrate all available knowledge on changes known to occur in the GI tract following bariatric surgery and can assist with dosage recommendation when there is an absence of clinical observations.

4.6 Conclusions

In this work we demonstrated the potential of a physiologically-based pharmacokinetic modelling and simulation to predict oral drug bioavailability post bariatric surgery by evaluating earlier developed models using observed data for cyclosporine and atorvastatin. Trends in oral drug exposure of atorvastatin and cyclosporine were predicted well within the 95% prediction interval following Roux-en-Y gastric bypass utilising the previously developed model at a small intestinal transit time of 3.0 hours. The results suggest a reduction in small intestinal transit time to be the most likely scenario following RYGB. The observed increase in atorvastatin exposure following biliopancreatic diversion with a duodenal switch could not be captured utilising the developed BPD-DS model incorporating all known physiological alterations.

A mechanistic PBPK modelling approach has the potential to serve as a tool in examining the impact of physiological alterations on oral drug bioavailability in the

absence of clinical data. The demonstrated approach may allow a framework for optimisation of oral drug therapy post bariatric surgery.

4.7 Acknowledgements

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4.8 Conflict of interest

The authors reported no conflicts of interest.

4.9 Study highlights

4.9.1 What is the current knowledge?

Patients undergoing bariatric surgery receive various therapeutic drugs. A limited number of studies have investigated oral drug exposure postoperatively. Bariatric surgery models were previously developed using the ADAM model within the PBPK simulator, Simcyp.

4.9.2 What question this study addressed?

We report on the evaluation of previously developed bariatric surgery PBPK models by comparing observed vs. predicted impact of surgery on oral exposure of cyclosporine and atorvastatin.

4.9.3 What this study adds to our knowledge

Trends in oral exposure of atorvastatin and cyclosporine were well predicted following RYGB. Observed increase in atorvastatin exposure following BPD-DS could not be captured using the current model.

4.9.4 How this might change clinical pharmacology and therapeutics

The potential of a PBPK modelling approach was demonstrated, allowing a framework for optimizing oral drug therapy post-bariatric surgery. Developed models integrated available knowledge on physiological changes. The study highlights areas of further research, where models are not predictive due to the lack of information on systems parameters.

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Chapter 5: Assessing the turnover of the intestinal epithelia in pre- clinical species and humans

Chapter 5: Assessing the turnover of the intestinal epithelia in pre-clinical species and humans

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In preparation

5.1 Abstract

Due to the rapid turnover of the small intestinal epithelia, the rate at which enterocyte renewal occurs plays an important role in determining the level drug-metabolising enzymes in the gut wall. Current physiologically-based pharmacokinetic (PBPK) models consider enzyme and enterocyte recovery as a lumped first-order rate. An assessment of the enterocyte turnover would allow enzyme and enterocyte renewal to be modelled more mechanistically. A comprehensive literature search together with statistical analysis was employed in order to establish the enterocyte turnover (or lifespan) in human and pre-clinical species. A total of 54 studies were identified reporting enterocyte turnover in 929 subjects in six species (mouse, rat, guinea pig, hamster, pig and human). In the mouse, the weighted combined geometric mean (WX) enterocyte turnover was 2.78 (± 1.06 , $n=113$) days. In the rat, the weighted arithmetic mean enterocyte turnover was determined to be 2.01 days ($n=287$). Combined human enterocyte turnover data ($n=265$) exhibited a WX turnover of 3.48 (± 1.55) days for the gastrointestinal epithelia, thus displaying comparable turnover to that of Cytochrome P450 enzymes as determined *in vitro* (0.96-4.33 days). Statistical analysis indicated that humans display a longer enterocyte turnover time as compared to pre-clinical species. Human data was too sparse to support regional differences in small intestinal enterocyte turnover despite being indicated in mouse. The utilisation of enterocyte turnover data, together with *in vitro* enzyme turnover, in PBPK modelling may be of assistance in improving predictions of drug-drug interactions and gastrointestinal metabolism in special populations where enterocyte turnover may be altered.

5.2 Introduction

Physiologically-based pharmacokinetic (PBPK) models of oral drug absorption and gut-wall metabolism may be implemented at a varying degree of complexity from simple first-order rate of absorption into the enterocytes to more sophisticated segmented models of the intestinal tract, such as the advanced compartmental absorption and transit (ACAT) model, advanced dissolution absorption and metabolism (ADAM) model and the segregated flow model (SFM); allowing the incorporation of segmentally segregated blood flows and regional variations in permeability, mucosal volumes and metabolic capacity (Agoram *et al.*, 2001; Pang, 2003; Darwich *et al.*, 2010). PBPK modelling of the oral component of drug bioavailability allows the estimation of the gut-wall extraction and further implementation to accommodate mechanistic prediction of drug-drug interactions (DDIs) in the small intestine, including: Reversible inhibition, mechanism-based inhibition (MBI) and enzyme induction (Fahmi *et al.*, 2009; Rowland Yeo *et al.*, 2010).

Furthermore, the utilisation of PBPK modelling and simulation of oral drug absorption processes enables the extrapolation of gastrointestinal drug disposition to special disease populations allowing the investigation drug-disease interactions where the metabolic capacity may be altered, such as post bariatric surgery or untreated coeliac disease (Johnson *et al.*, 2001; Darwich *et al.*, 2012; Darwich *et al.*, 2013).

Dynamic modelling of intestinal metabolism requires knowledge of the level of enzyme in the gut-wall where the amount of active enzyme at steady state is a product of rate of synthesis and degradation, a process generally referred to as turnover. Enzyme turnover plays an important role in the pharmacokinetic outcome and model-based prediction of MBIs and enzyme induction in the small intestine, where the reliance upon small intestinal enzyme turnover becomes especially apparent for drugs exhibiting high small intestinal metabolism and for substrates of cytochrome P450 (CYP) 3A, being the most abundant enzyme in the gut (Yang *et al.*, 2008).

Current PBPK models do not account for the nesting of enzyme turnover and enterocyte turnover and instead utilises a lumped first-order enzyme turnover rate informed via indirect measures, such as clinical MBI studies. Accounting for the nesting of enzyme turnover within the enterocytes may provide a framework for improved predictions of

mechanism-based inhibition, enzyme induction, and special subpopulations where the turnover may potentially be altered. The utilisation of enterocyte turnover does however require the data to inform such parameters. Where earlier research has characterised the indirect and *in vitro* enzyme turnover utilising meta-analysis no similar efforts have been made to establish enterocyte turnover (Yang *et al.*, 2008).

Physiologically, the enterocytes are produced through cell division of progenitor stem cells in the crypt at the base of the villi in the intestinal tissue. These progenitor cells are subject to proliferation into enterocytes and other functional cells through cell division. Mature enterocytes will migrate up the crypt-villous axis where the turnover will be governed by apoptosis and shedding into the gut lumen at the tip of the villi. The time from enterocyte generation to shedding will occur within days after proliferation (Wilson and Potten, 2004; Malato *et al.*, 2011).

The aim of the current study was to assess the enterocyte turnover in pre-clinical species and human and to identify the most commonly utilised methods for determining enterocyte turnover.

5.3 Methods

A comprehensive literature search was performed in order to identify published data on direct determination of full small intestinal (duodenum, jejunum and ileum) enterocyte turnover, lifespan, cell cycle or migration rate in healthy adults in preclinical species (including: rat, mouse, pig, dog, guinea pig, rabbit and hamster) as well as methods utilised to determine the turnover, using PubMed (1950-2013). For human data the literature was extended to include gastric, colonic and rectal epithelial cells and patient populations due to the sparsity of data. Additional sources were identified through publication citations for all species.

Collated data was analysed using descriptive statistics, calculating weighted arithmetic means (WX) utilising reported means (x_i) and sample size (n_i) of individual studies (Equation 5.1). Studies reporting mean data only where n_j was not clearly stated were penalised assuming $n_j = 1$; whereas for studies where the mean and standard deviation were reported without clearly stating n_j were assigned $n_j = 3$. The combined standard

deviation (overall SD) was obtained through calculating the total sum of squares (overall SS) (Equation 5.2 and Equation 5.3). When data allowed, the geometric mean (GM) and geometric standard deviation (GSD) of the enterocyte turnover were calculated by calculating σ (lnSD; Equation 5.4 and Equation 5.5), using the reported mean and variance and μ (lnGM; Equation 5.6 and Equation 5.7). Statistical analysis was carried out to test for regional and interspecies differences in enterocyte turnover using Welch's t test ($P < 0.05$) with post-hoc Dunn-Šidák correction in Matlab® R2010a (Mathworks, Natick, USA) using sample means (X), size (n) and standard deviations (s^2) where data allowed (Equation 5.8).

$$WX = \frac{\sum_{i=1}^n n_i \cdot X_i}{\sum_{i=1}^n n_i}$$

Equation 5.1. Weighted mean.

$$Overall\ SS = \sum_{i=1}^n [(SD_i^2 + X_i^2) \cdot n_i] - N \cdot WX^2$$

Equation 5.2. Overall sum of squares.

$$Overall\ SD = \sqrt{\frac{Overall\ SS}{N}}$$

Equation 5.3. Overall standard deviation.

$$\sigma = \sqrt{\ln\left(\frac{variance}{X^2} + 1\right)}$$

Equation 5.4. logarithmic standard deviation.

$$GSD = e^{\sigma}$$

Equation 5.5. Geometric standard deviation.

$$\mu = \ln X - \frac{1}{2} \cdot \ln\left(\frac{1}{2} \cdot \sigma^2\right)$$

Equation 5.6. Logarithmic mean.

$$GM = e^{\mu}$$

Equation 5.7. Geometric mean.

$$t = \frac{X_1 - X_2}{\sqrt{\frac{s_1^2}{N_1} - \frac{s_2^2}{N_2}}}$$

Equation 5.8. Welch's t test.

5.4 Results

Overall, a total of 54 studies were identified reporting enterocyte turnover in 954 subjects in 6 species. In a majority of the studies determination of enterocyte turnover was carried out using isotope labelling utilising ^3H -thymidine or BrdUrd (81%), the remainder were carried out using techniques such as mitotic arrest methods with colchicine and vincristine, and turnover determination in biopsy samples. Underneath follows an account for some of the most common methods for determining enterocyte turnover.

5.4.1 *Methods for determining the turnover of enterocytes*

Various *in vivo* and *in vitro* methods exist for determining the turnover of the enterocytes where many of these remain consistent across different tissues. The small intestinal epithelia differ from other physiological cell lines in the sense that it is a highly organised tissue allowing the study of cell migration within the tissue (Wilson and Potten, 2004).

Isotope labelling methods

The most commonly used method for measuring enterocyte turnover is the 'pulse-chase' method, where the DNA of a population of cells is labelled with an isotopic nucleoside, such as ^3H -thymidine, or a synthetic isotopic analogue such as bromodeoxyuridine (BrdUrd). Following administration of the isotopic nucleotide the

label will incorporate into the DNA during the synthetic phase (S-phase). The cell line can be monitored post labelling using autoradiography as cells are progressing through their life cycles, thus allowing quantitative determination of the time span of these different phases (Figure 5.1) (Quastler and Sherman, 1959; Creamer, 1967; Scragg and Johnson, 1980).

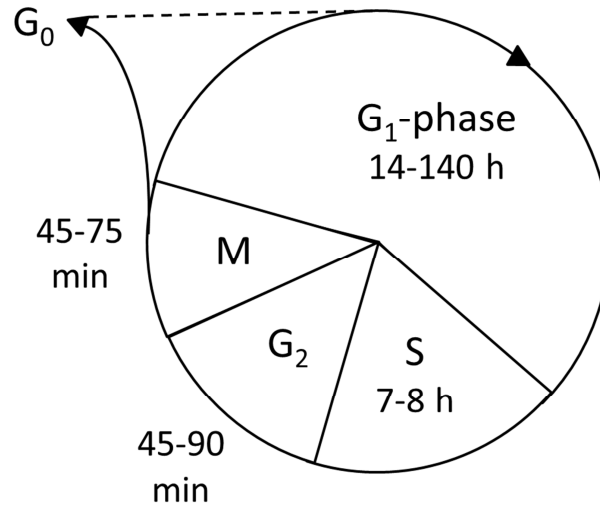


Figure 5.1. Schematic of the phases of the enterocyte cell cycle, characterised by: The time between mitosis and DNA synthesis (G₁: 14-140 h), DNA synthesis (S: 7-8 h), time between DNA synthesis and mitosis (G₂: 45-90 min) and mitosis (M: 45-74 min). Adapted from Scragg and Johnson, 1980 (Scragg and Johnson, 1980).

With knowledge of the duration of the S-phase (T_S) and the labelling index of the cell population (LI), the turnover of a cell line can be determined *in vitro* or *in vivo*, where the turnover time (T_{ot}) is equal to the ratio (reported as a percentage) of the T_S and LI (Equation 5.9 and Figure 5.2) (Scragg and Johnson, 1980).

$$T_{ot} = \frac{T_s}{LI} \cdot 100$$

Equation 5.9. Determination of turnover time.

Due to the high organisation of the intestinal tissue, the turnover of the enterocytes can be determined by estimating the migration time of cells from the villous-crypt junction

to the tip of the villous if the height of the villous is determined. The migration time will be equal to the enterocyte lifespan and thus the turnover of the small intestinal epithelia (Leblond and Stevens, 1948).

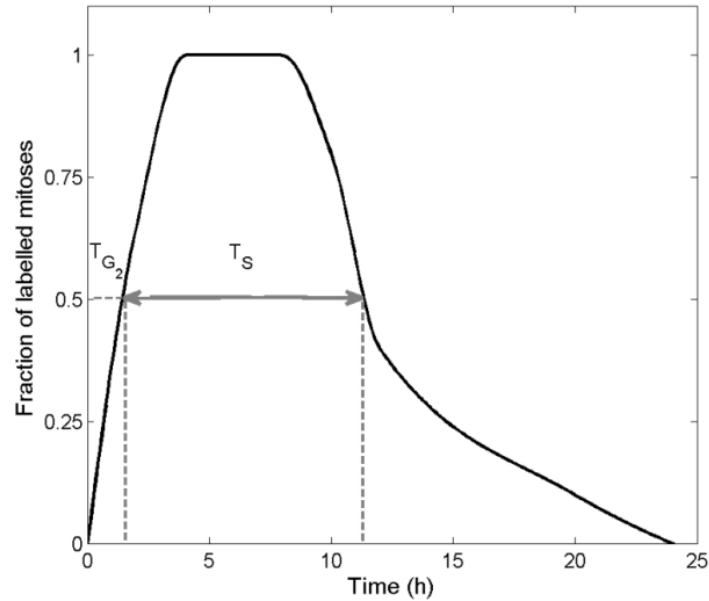


Figure 5.2. Conceptual figure of the fraction of labelled mitoses against time following the isotope labelling, indicating the length of the G_2 and S-phase (T_{G_2} and T_S), thus allowing the determination of cell turnover time. Adapted from Scragg and Johnson 1980 (Scragg and Johnson, 1980).

Mitotic arrest methods

The mitotic arrest methods involve stathmokinetic agents (such as: colchine, colcemid, vinblastine or vincristine) arresting cells in the metaphase entering mitosis. This will result in an accumulation of the mitotic figures, allowing the determination of the number of cells in metaphases by histological examination. The mitotic arrest technique can be used *in vitro*, or *in vivo* by administering the blocking agent via intravenous or intraperitoneal injection (Scragg and Johnson, 1980).

Cell production rate can be determined from the relation between the number of cells in metaphase against time. The relation can be used to estimate the cell cycle times as the inverse relation of the rate of cells entering mitosis (Equation 5.10) (MI_s/t).

$$T_c = \frac{1}{MI_s/t}$$

Equation 5.10. Cell production rate.

Additionally, the villous transit time can be determined as a ratio between the villous population and the cell influx per villous (Equation 5.11) (Al-Nafussi and Wright, 1982).

$$Transit\ time = \frac{Villous\ population}{Cell\ influx/villous}$$

Equation 5.11. Enterocyte transit time.

Cytophotometric methods

Cytophotometric methods involve the staining of the cell line DNA using dyes, such as ethidium bromide, which bind specifically to DNA and fluoresce with intensity proportional to the amount of bound DNA. This allows the distinguishment between cell cycle states and the proliferative index of a population, percentage in D G2 and M phase (Scragg and Johnson, 1980).

5.5 Results

Overall, a total of 53 studies were identified reporting enterocyte turnover in 929 subjects in 6 species. In a majority of the studies determination of enterocyte turnover was carried out with isotope labelling utilising ³H-thymidine or BrdUrd (83%), where other techniques included mitotic arrest methods with colchicine and vincristine, and turnover determination using biopsy samples. The outcome of the data analysis of enterocyte turnover follows below.

5.5.1 Enterocyte turnover in pre-clinical species

The literature search of enterocyte turnover in healthy adult subjects of pre-clinical species identified a total of 36 studies, consisting of approximately 664 subjects based on sample size assumptions given in the Methods section. In the rat, 14 studies

consisting of 262 subjects were identified, where the weighted arithmetic mean full small intestinal enterocyte turnover (*i.e.* lifespan) was determined to be 2.01 days. Values for segmental turnover of the small intestinal epithelia were within close proximity of each other with weighted averages of 1.89, 2.11 and 1.91 days, in the duodenum, jejunum and ileum respectively. Estimates of variability were limited to two radiographic studies of the duodenum and jejunum reporting standard deviations of the mean turnover. The weighted geometric mean and standard deviation of these reports resulted in an enterocyte turnover corresponding to 2.76 (± 1.68) days (n rats=14). Due to the limited reported variance statistical verification of regional differences was restricted, albeit reported turnover in the duodenum (1.20 ± 0.20 days, n=4) and jejunum (3.95 ± 0.54 days, n=10) displayed a statistically significant difference ($P < 0.05$) (Figure 5.3) (Leblond and Stevens, 1948; Bertalanffy, 1960; Loran and Althausen, 1960; Bertalanffy and Lau, 1962; Koldovsky *et al.*, 1966; Altmann and Enesco, 1967; Shambaugh *et al.*, 1967; Menge *et al.*, 1982; Holt *et al.*, 1983; King *et al.*, 1983; Cheeseman, 1986; Nsi-Emvo *et al.*, 1994; Thomson *et al.*, 1994; Gomes and Alvares, 1998; Macallan *et al.*, 1998; Qi *et al.*, 2009).

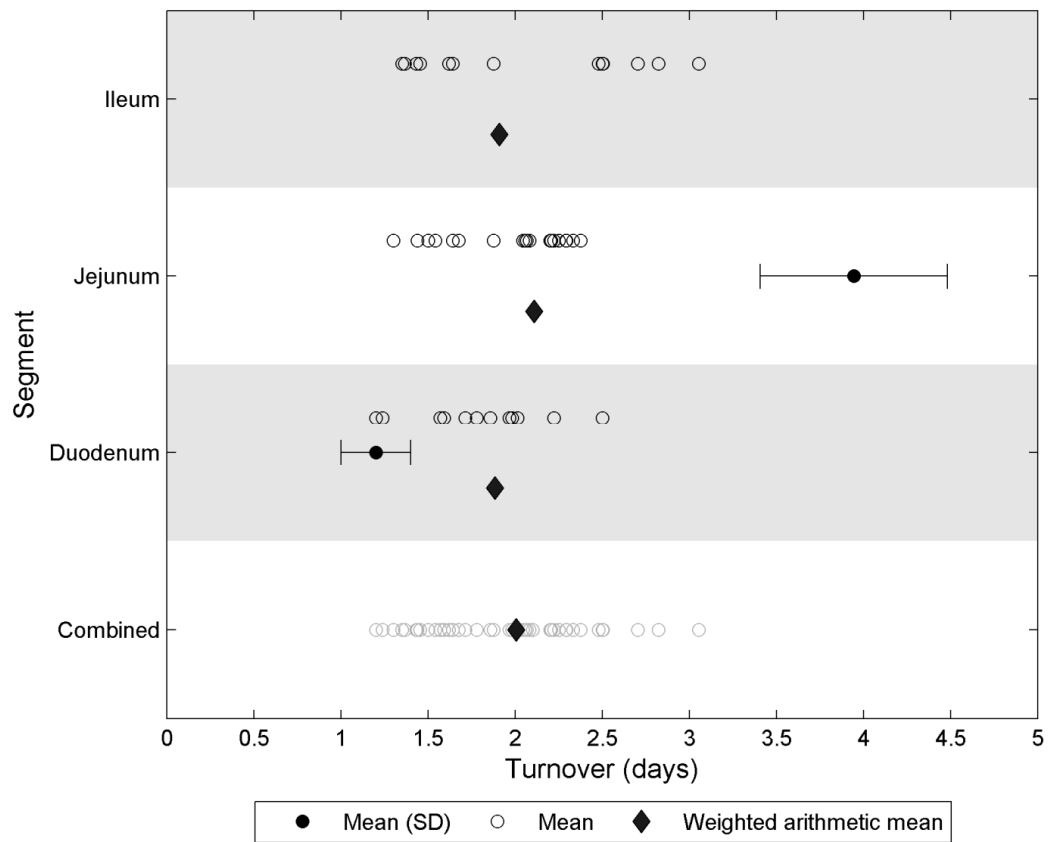


Figure 5.3. Reported means and standard deviations (SD; n rats=14) and mean only data (n=248) of small intestinal enterocyte turnover in rat and the combined weighted geometric mean and SD (GSD) based on dataset of mean and SD.

In the mouse, a total of 15 studies consisting of 373 healthy adult mice were identified reporting the enterocyte turnover in the small intestinal epithelia. The weighted combined geometric mean full enterocyte turnover for the whole small intestine was 2.78 (± 1.06 n=113 mice) days. The duodenum, jejunum and ileum displayed an enterocyte turnover of 2.83 (± 1.06 , n=40), 2.97 (± 1.05 , n=35) and 2.56 (± 1.05 , n=35) days respectively. All intestinal segments differed at a statistically significant level using post-hoc analysis ($P < 0.05$) (Figure 5.4) (Leblond and Messier, 1958; Walker and Leblond, 1958; Quastler and Sherman, 1959; Fry *et al.*, 1961; Leshner *et al.*, 1961; Fry *et al.*, 1962; Grey, 1968; Merzel and Leblond, 1969; Cheng and Leblond, 1974; Tsubouchi, 1981; Cheng and Bjerknes, 1983; Smith *et al.*, 1984; Thompson *et al.*, 1990; Ferraris *et al.*, 1992).

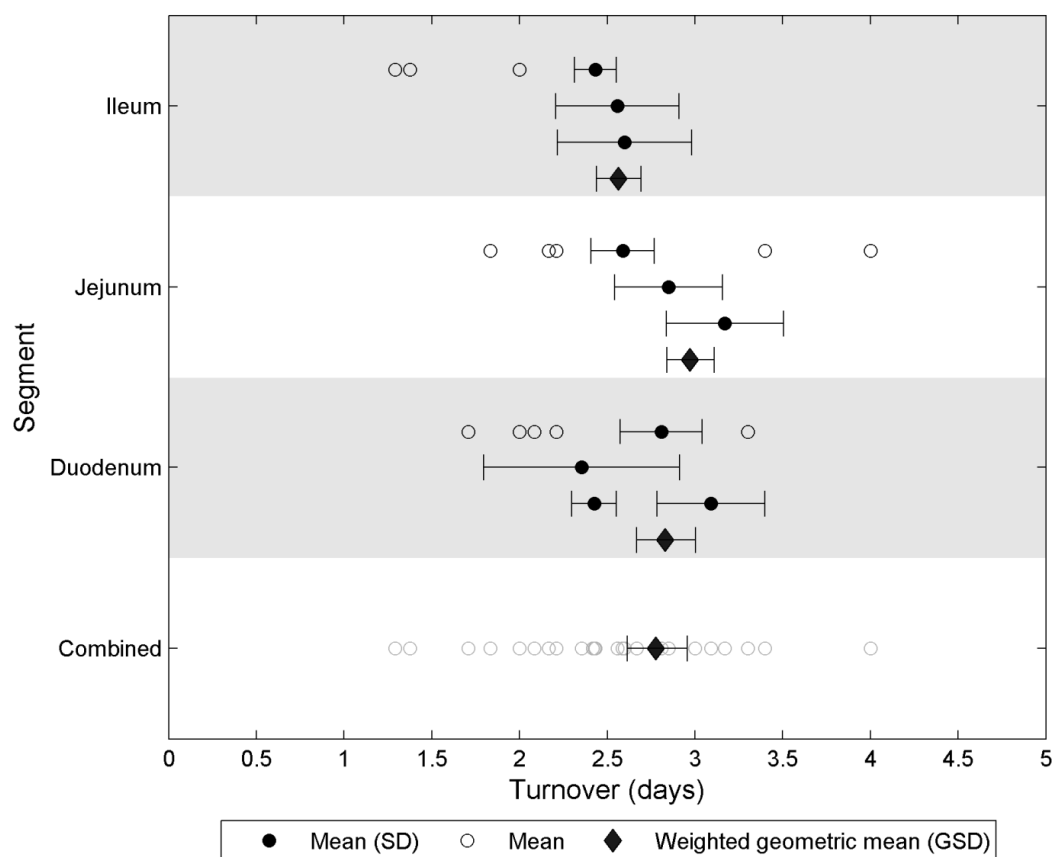


Figure 5.4. Reported means and standard deviations (SD; n=113 mice) and mean only data (n=260) of small intestinal enterocyte turnover in the mouse and the combined weighted geometric mean and SD (GSD) based on dataset of mean and SD.

5.5.2 Enterocyte turnover in human

The literature search of human enterocyte turnover data identified 17 studies, with a total sample size of n=265, reporting the turnover of human gastrointestinal epithelial cells in the form of mean and standard deviation (n=86), mean only (n=153) and ranges (n=26). The majority of turnover values were from colonic, rectal (n=157), duodenal (n=60) and gastric epithelial cells (n=36), whereas jejunum and ileum was limited to a sample size of n=3 and n=9 respectively. A weighted geometric mean turnover of 3.48 (± 1.55) days was obtained for the gastrointestinal epithelia, limiting analysis to data reporting the mean and standard deviation. Analysis of individual gastrointestinal segments identified a weighted mean turnover of 1.50 (± 2.90 , n=3) days for the duodenum, 2.83 (± 1.60 , n=30) days for the stomach and 4.12 (± 1.32 , n=53) days for the colorectal region, where the stomach displayed a statistically faster turnover as

compared to the colorectal region utilising post-hoc test ($P<0.05$) (Figure 5.5) (Bertalanffy and Nagy, 1961; Cole and Mc, 1961; Deschner *et al.*, 1963; Lipkin *et al.*, 1963a; Lipkin *et al.*, 1963b; Macdonald *et al.*, 1964; Shorter *et al.*, 1964; Shorter *et al.*, 1966; Bell *et al.*, 1967; Lipkin, 1969; Bleiberg *et al.*, 1970; Weinstein, 1974; Bleiberg and Galand, 1976; Wright *et al.*, 1977; Potten *et al.*, 1992; Patel *et al.*, 1993; Bullen *et al.*, 2006).

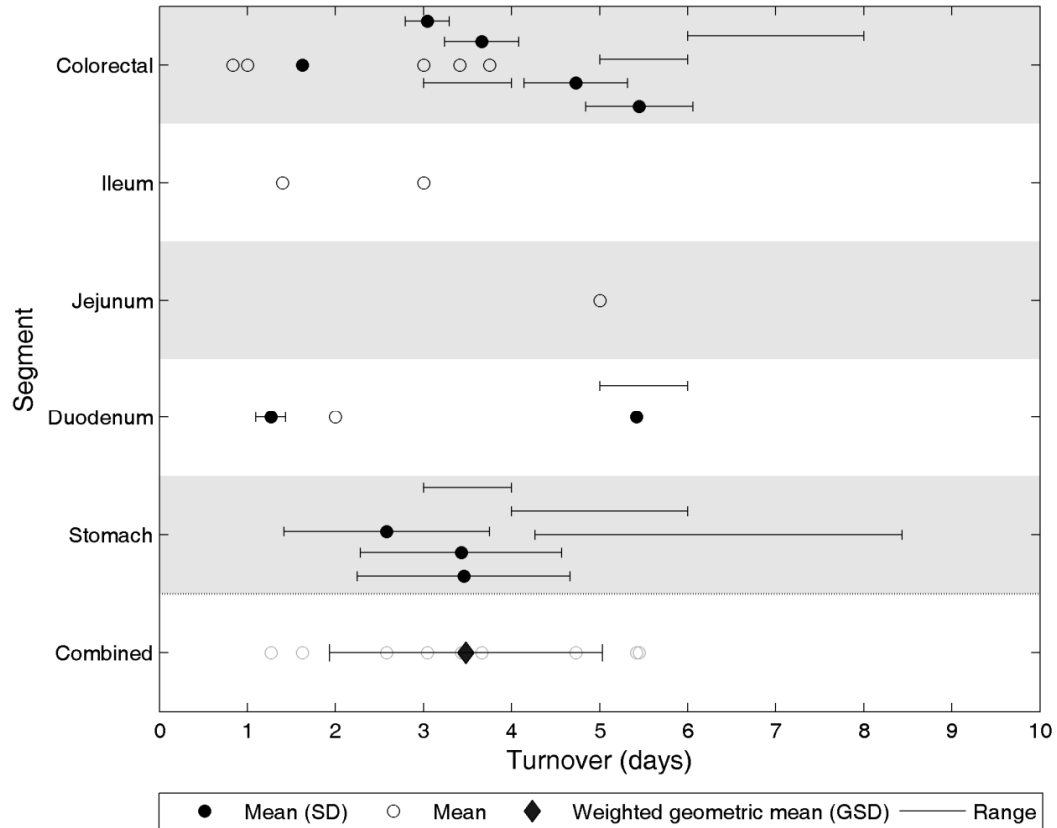


Figure 5.5. Reported means and standard deviations (SD; n individuals=86), mean only data (n=153), and ranges (n=26) of human gastrointestinal epithelial turnover and the combined weighted geometric mean and geometric SD (GSD; n=86) based on dataset of mean and SD.

5.5.3 Summary results on enterocyte turnover

In addition to human, rat and mouse, data on small intestinal enterocyte turnover was identified for healthy adult rabbits, guinea pigs and hamsters, albeit being sparse. The arithmetic mean enterocyte turnover in rabbit, guinea pig and hamster corresponded to 3.40 (n=20 rabbits), 3.38 (n=Not clear) and 1.67 (n=8) days respectively. Statistical analysis of enterocyte turnover in human, mouse and rat identified human and mouse enterocyte turnover to differ statistically significantly ($P<0.05$) (Figure 5.6) (Cremaschi *et al.*, 1982; Cremaschi *et al.*, 1984; Smith *et al.*, 1984).

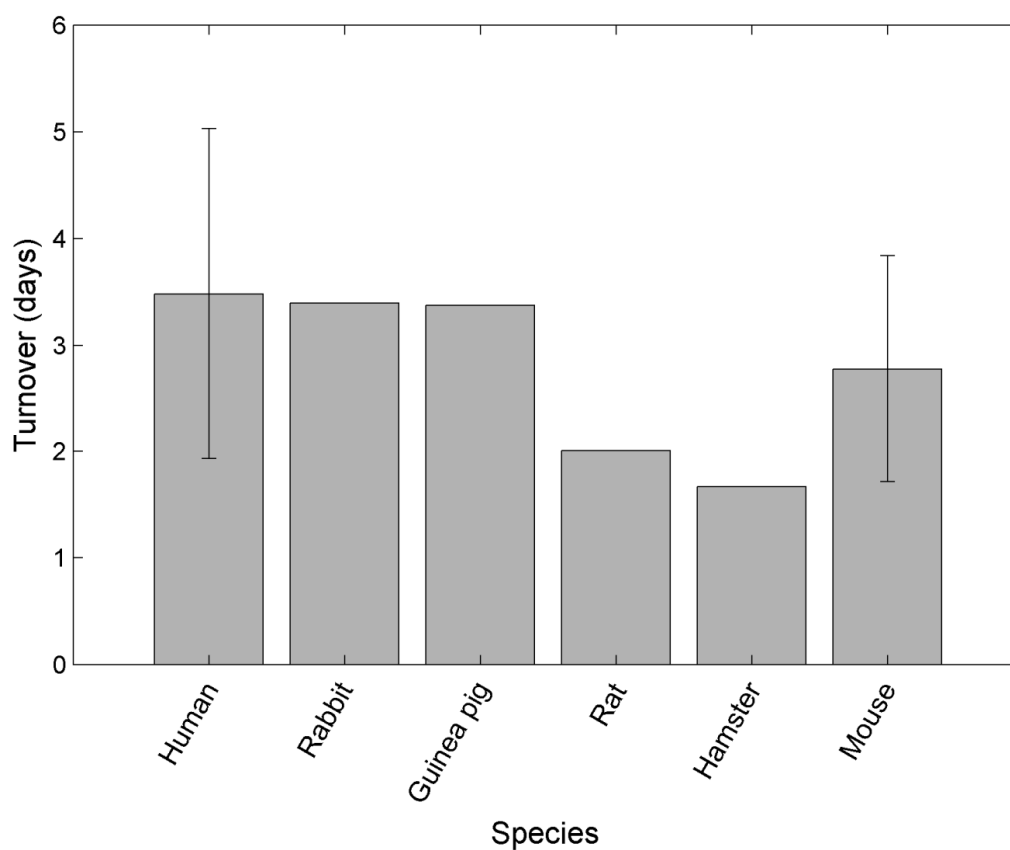


Figure 5.6. Reported enterocyte turnover in days across species, ranked approximately according to body weight, in: Human (n individuals=86), rabbit (n =20), guinea pig (n=Not clear), rat (n=262), hamster (n=8) and mouse (n=131).

5.6 Discussion and conclusions

Turnover of the gastrointestinal epithelia was established based on large sample size in rats, mice and human and based on sparse samples in rabbits, guinea pig and hamster. Statistical analysis indicated a shorter enterocyte turnover in preclinical species as compared to human, where the mouse displayed a significantly shorter turnover, albeit the limitation of data did not allow a conclusive analysis for the remaining species. It should further be noted that human data included gastric and colorectal epithelial turnover data due to the sparse dataset from the small intestinal region.

Statistical analysis of regional differences in enterocyte turnover indicated the ileum to display the fastest turnover, followed by the duodenum and ileum in mouse. A similar trend was indicated in rat although a majority of the data lacked variance and could therefore not be determined statistically. Human data on gastrointestinal epithelial turnover identified the colorectal cell renewal to be slower as compared to the stomach, whereas data from the small intestinal regions were too sparse in order to observe any regional differences. Additional indications of regional differences in enterocyte turnover include observations from neonatal pig, where the distal small intestine displayed a slower turnover (10.2 ± 1.5 days, $n=16$) as compared to the proximal region (4.7 ± 0.4 days, $n=16$) (Fan *et al.*, 2001). In summary, evidence for regional differences in enterocyte turnover in man is inconclusive which would favour the utilisation of a single parameter value of 3.48 (± 1.55) days for the intestine.

Several factors have been identified to alter the turnover of the enterocytes, and may therefore account for variability seen in the data set, these factors include the age of the subjects, where several reports have reported slower enterocyte turnover in neonatal or infant pigs, guinea pigs, rats, mice and hamsters (Creamer *et al.*, 1961; Koldovsky *et al.*, 1966; Grey, 1968; Rundell and Lecce, 1972; Al-Nafussi and Wright, 1982; Holt *et al.*, 1983; Cremaschi *et al.*, 1986; Fan *et al.*, 2001; Leaphart *et al.*, 2008). In addition, an altered enterocyte turnover has been reported in rats subject to numerous environmental changes and disease states, including: Small intestinal resection, dietary changes, diabetes and irradiation (Menge *et al.*, 1982; Menge *et al.*, 1983; Cheeseman, 1986; Thomson *et al.*, 1994). It can therefore be concluded that the enterocyte turnover is highly sensitive to numerous environmental factors.

The quality of data posed the perhaps most significant limitation in this study, with a large number of studies only reporting mean data or ranges of enterocyte turnover, this was especially true for the human data where labelling studies tend to be performed in colorectal cancer patients, this may further influence the turnover. A majority of human data therefore originated from the colorectal and gastric region, which should be taken into consideration when interpreting interspecies differences in enterocyte turnover as reported in this study.

The enterocyte turnover, as determined in this analysis (approximately 3.48 days), suggests the gastrointestinal epithelia to display a comparable rate of renewal to that of the CYP enzymes as determined *in vitro*, where Yang, and co-workers, found reported CYP turnover vary between 0.96 and 4.33 days. The individual impact of these two hierarchically dependent processes on enzyme recovery following DDIs is however not completely straightforward to compare as the rate of turnover of the enzymes will follow a first-order rate following mechanism-based inhibition whereas the enterocytes can be assumed to be renewed at a zero-order rate as steady-state levels of the enterocyte population remain undisrupted following inhibition. Exploring the impact of nesting enzyme and enterocyte turnover for the prediction of DDIs and MBI may be considered particularly suitable using a PBPK modelling and simulation approach (Bell *et al.*, 1967; Yang *et al.*, 2008; van Leeuwen *et al.*, 2009).

This is the most extensive analysis of enterocyte turnover in multiple species, including human, to the authors' knowledge. The incorporation of enterocyte turnover data in PBPK modelling and simulation may be of assistance in improving the predictions of DDIs where substrates are subject to small intestinal metabolism through the incorporation of independent enterocyte and enzyme turnover in the gut wall, thus allowing a more mechanistic description of the recovery of enzyme following MBI or induction or disease states where enzyme or enterocyte turnover are altered independently.

5.7 Acknowledgements

The Authors declare no conflict of interest.

5.8 References

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**Chapter 6: Development and
assessment of a nested enzyme-
within-enterocyte turnover model
for mechanism-based inhibition
in the small intestine**

Chapter 6: Development and assessment of a nested enzyme-within-enterocyte turnover model for mechanism-based inhibition in the small intestine

A.S. Darwich, D.M. Ashcroft, A. Rostami-Hodjegan

6.1 Abstract

The extent of mechanism-based inhibition (MBI) of gut wall metabolism depends upon the degradation and synthesis of drug metabolising enzymes ($k_{deg,Enz}$) as well as the turnover rate of the enterocytes ($k_{deg,Ent}$). Current models do not consider the hybrid function determining $k_{deg,Enz}$ and instead utilise surrogate markers. Considering the complexity of the hybrid function would potentially improve the prediction of MBIs in the gut wall.

A 'nested enzyme-within-enterocyte' (NEWE) model describing Cytochrome P450 (CYP) 3A4 dynamics in the gut wall was developed using Matlab[®] R2010a (Mathworks, Natick, USA). A sensitivity analysis was carried out, exploring the impact of realistic ranges of MBI parameters on the extent of interaction, including: The maximal rate of enzyme inactivation (k_{inact}), unbound inhibitor concentration producing half of the maximal rate of inactivation ($K_{I,u}$), the turnover rate of the enterocytes ($k_{deg,Ent}$) and CYP3A4 ($k_{deg,CYP3A}$).

The conventional modelling approach ($k_{deg,Ent}=0\text{ h}^{-1}$) led to a higher level of inhibition of small intestinal CYP3A4 activity following MBI as compared to the NEWE model. The lower range of $K_{I,u}$'s or a higher k_{inact} were more likely to be associated with a higher predicted interaction following MBI when using the conventional model as compared to the NEWE model after single dose of inhibitor. Following multiple dose, a low k_{inact} and medium $K_{I,u}$ produced the highest discrepancy between the two models. The NEWE model may partly explain the commonly reported overpredictions of small intestinal inhibition seen for MBI when utilising the conventional modelling approach and may further improve the prediction of moderate to high MBIs. Parameter estimations of $k_{deg,CYP3A}$ based on clinical studies involving CYP3A4 MBI may be inaccurate without considering the $k_{deg,Ent}$.

6.2 Introduction

Intestinal metabolism plays an important role in the first-pass of orally administered drugs. The small intestine has been shown to exhibit comparable metabolic capability to the liver, where cytochrome P450 3A4 (CYP3A4) is the most abundant drug metabolising enzyme (Thelen and Dressman, 2009).

In physiologically-based pharmacokinetic (PBPK) modelling of intestinal first-pass, metabolism is treated as the net intrinsic unbound clearance ($CL_{u,int,G}$) often occurring inside a "well-stirred" gut model or the Q_{gut} model, where the flow from the enterocyte is treated as a hybrid term of permeability and villous blood flow (Yang *et al.*, 2007). More mechanistic models describing oral drug bioavailability generally include a series of intestinal gut wall compartments to accommodate the regional variation in enzyme abundances and segmental segregated villous blood flows, examples of these models include: The advanced compartmental absorption and transit (ACAT) and advanced dissolution absorption and metabolism (ADAM) models (Agoram *et al.*, 2001; Yang *et al.*, 2007; Jamei *et al.*, 2009; Gertz *et al.*, 2011).

Prediction of drug-drug interactions (DDIs), such as mechanism-based inhibition (MBI), through the utilisation *in vitro-in vivo* extrapolation (IVIVE) is an essential application of PBPK modelling and simulation. In order to predict MBI, PBPK models rely on a set of inhibitor and systems specific parameters, where the level of active enzyme over time in the small intestine (A_{Enz-GI}) will depend upon the unbound inhibitor concentration in the enterocytes ($fu_{Ent} \cdot I_{Ent}$), its maximal rate of enzyme inactivation (k_{inact}) and the inhibitor concentration that produces half of the maximal rate of inactivation ($K_{I,u}$). The level of interaction will further be determined by the level of active enzyme at steady state ($A_{Enz-GI,SS}$) and the effective enzyme degradation rate ($k_{deg,Enz}$) (Equation 6.1) (Rowland Yeo *et al.*, 2010).

$$\frac{dA_{CYP-GI}}{dt} = k_{deg,Enz} \cdot A_{Enz-GI,SS} - A_{Enz-GI} \cdot \left(k_{deg,Enz} \cdot \frac{k_{inact} \cdot fu_{Ent} \cdot I_{Ent}}{K_{I,u} + fu_{Ent} \cdot I_{Ent}} \right)$$

Equation 6.1. Mechanistic model of mechanism-based inhibition.

The systems parameter $k_{\text{deg,Enz}}$, a surrogate parameter of the combined turnover rate of the enterocyte and enzyme, is crucial in determining the timeframe and extent at which the MBI will occur (Equation 6.2) (Yang *et al.*, 2008).

$$R_{\text{syn}} = A_{\text{CYP-GI,SS}} \cdot k_{\text{deg-CYP}}$$

Equation 6.2. Enzyme turnover.

Due to the rapid turnover of the gastrointestinal epithelium compared to other tissues the enzyme turnover in the intestine will highly depend on the enterocyte lifespan (between 1-7 days in man), as opposed other cell tissues with metabolic capabilities, such as the hepatocytes (approximately 200-400 days in rat and mouse) (Malato *et al.*, 2011).

In vivo methods for determining $k_{\text{deg-Enz}}$ through measuring the recovery time of enzyme activity following enzyme the MBI are confounded by the turnover of the enterocytes; whereas *in vitro* data of enzyme degradation are sparse (Yang *et al.*, 2008).

Techniques for measuring cell turnover often rely on the incorporation of a label into the intracellular DNA. Non-radioactive labeling techniques where label compounds, such as bromodeoxyuridine and iododeoxyuridine, are administered as a single pulse label together with flow cytometry have enabled the examination of cell kinetics to a wider extent both *in vivo* and *in vitro* (Rew and Wilson, 2000).

A reoccurring problem exists in the prediction of the magnitude of mechanism-based inhibition (MBI) where overestimations of DDIs have been reported repeatedly, in particular for drugs exhibiting high intestinal extraction. Despite the improved predictions of DDIs using more mechanistic approaches, several examples of over-predictions exist, including fluoxetine and mibefradil (Obach *et al.*, 2007; Galetin *et al.*, 2008; Fahmi *et al.*, 2009; Burt *et al.*, 2012).

A systems pharmacology modelling approach to nesting enzyme-within-enterocyte turnover would provide a more mechanistic framework for modelling the physiological factors involved in the recovery of enzyme activity over time following MBI by taking

enzyme and enterocyte turnover into account and thus has the potential to improve the predictions of MBI in the gut wall.

The aim was to theoretically examine the nesting and hierarchy of enterocyte and CYP3A4 enzyme turnover and its impact on MBIs in the small intestine using a systems pharmacology approach. This would be carried out through the development and assessment of a nested enzyme-within-enterocyte (NEWE) model.

6.3 Materials and Methods

A nested enzyme-within-enterocyte (NEWE) turnover model describing CYP3A4 activity in the gastrointestinal tract was developed using Matlab[®] R2010a combined with the C programming language.

Realistic parameter estimates and ranges of $k_{\text{deg-Ent}}$, the degradation rate of small intestinal CYP3A4 ($k_{\text{deg-CYP3A}}$), K_{inact} and $K_{\text{I,u}}$, were explored through a simulation based exploratory sensitivity analysis utilising the developed NEWE model. The range of the explored parameter space of $k_{\text{deg-CYP3A}}$ was based on CYP3A4 turnover data extracted from the review by Yang, and co-workers, 2007 (Yang *et al.*, 2007). Ranges of explored K_{inact} and K_{I} values were extracted from the review of MBIs by Zhou, and co-workers, 2005 (Zhou *et al.*, 2005). $K_{\text{I,u}}$ was estimated from the fraction of unbound drug in the inhibitory assay (fu_{mic}), this was estimated from drug dependent chemical descriptors (logP and logD) and microsomal assay protein concentrations (C_{mic}) obtained from relevant studies. If no information regarding C_{mic} was given a value of 0.1 mg/mL was assumed (Equation 6.3) (Austin *et al.*, 2002).

$$fu_{\text{mic}} = \frac{1}{C_{\text{mic}} \cdot 10^{0.56 \cdot \log P / D - 1.41} + 1}$$

Equation 6.3. Estimation of fu_{mic} .

An additional set of simulations were carried out for identified geometric mean values of $k_{\text{deg,Ent}}$, based on literature search carried out by Darwich, and co-workers, and $k_{\text{deg,CYP3A}}$, based on *in vitro* data, using the NEWE model as compared to the surrogate $k_{\text{deg,CYP3A}}$ ($k_{\text{deg,Ent}}=0 \text{ h}^{-1}$) (Yang *et al.*, 2008).

The dose level was determined based on the average dose of the 17th World Health Organisation (WHO) Model List of Essential Medicines (n drugs=135). Absorption rate (k_a) was based on the average of readily available reported k_a values from published population pharmacokinetic studies in human for drugs included in the 17th WHO model list of Essential Medicines (n drugs=74) (see supplementary material) (WHO, 2011).

The simulated outcome of the sensitivity analysis was examined by comparing the ratio of relative activity of CYP3A4 following MBI using the NEWE model as compared to corresponding $k_{deg,CYP3A}$ using the conventional model ($k_{deg,Ent}=0 \text{ h}^{-1}$) up to 240 hours ($A_{Ent-n/0,0-t} [\%]$; Equation 6.4).

$$A_{Ent-n/0,0-t} = \frac{A_{CYP3A4,0-t} k_{deg,Ent-n}}{A_{CYP3A4,0-t} k_{deg,Ent-0}}$$

Equation 6.4. Ratio of relative enzyme activity.

6.4 Results

A nested enzyme-within-enterocyte model was developed and utilised to explore the impact of $k_{deg-Ent}$ and $k_{deg-CYP3A}$ on mechanism-based inhibitor specific parameters k_{inact} and $K_{I,u}$ through sensitivity analysis. The results follow below.

6.4.1 Model specification

The time dependent amount of active CYP3A4 in the small intestine ($A_{CYP3A-GI}$) as a consequence of MBI was described in accordance to Equation 6.1 where the level of active enzyme ($A_{CYP3A-GI}$) will depend on the unbound inhibitor concentration in the enterocytes ($f_{u,Ent} \cdot I_{Ent}$), its maximal rate of enzyme inactivation ($k_{inact-CYP3A}$) and the inhibitor concentration that produces half of the maximal rate of inactivation ($K_{I,u-CYP3A}$). The level of interaction is further dependent on the level of active enzyme at steady state ($A_{CYP-GI,ss}$), the effective CYP degradation rate ($k_{deg-CYP}$), which in the proposed model is a product of enzyme degradation alone (Equation 6.5).

$$\frac{dA_{CYP3A-GI}}{dt} = k_{deg-CYP} \cdot A_{CYP3A-GI,SS} - \frac{\sum_{i=1}^N A_{CYP-GI,i}}{N} \cdot \left(k_{deg-CYP} \cdot \frac{k_{inact-CYP3A} \cdot fu_{Ent} \cdot I_{Ent}}{K_{lu-CYP3A} + fu_{Ent} \cdot I_{Ent}} \right)$$

Equation 6.5. NEWE model (1): Level of active enzyme.

The progression of the enterocyte lifecycle was described utilising a zero order growth rate ($k_{deg,ent}$) equal to the rate of enterocyte turnover ($T_{tot,ent}$) where a lifespan of one was assumed (Equation 6.6).

$$k_{deg,ent} = \frac{1}{T_{tot,ent}}$$

Equation 6.6. Definition of enterocyte zero-rate turnover.

The initial starting point of the enterocyte lifespan at time zero was determined by a pseudorandom generation between zero and one from a uniform distribution at the initially simulated time point ($A(0)_{Ent-Lifespan}$) (Equation 6.7).

$$\frac{dA_{Ent-Lifespan}}{dt} = A(0)_{Ent-Lifespan} + k_{deg-Ent}$$

Equation 6.7. NEWE model (2): Enterocyte lifespan.

The time dependent turnover of enterocytes was modelled using an event algorithm, where the amount of active CYP3A4 one enterocyte ($A_{CYP3A-GI,j}$) was dependent on its enterocyte life progression ($A_{Ent-Lifespan,j}$) increasing at a zero order rate equal to $k_{deg,ent}$. An $A_{Ent-Lifespan,j}$ equal to one equated cell apoptosis or shedding. The enterocyte was replaced by a new enterocyte starting at a life progression of zero and an amount of CYP3A4 equal to its steady state abundance. Thus governing the lifespan of the total population of enterocytes ($A_{Ent-Lifespan,N}$) and consequently the total amount of CYP3A4 in the small intestine ($A_{Ent-Lifespan,N}$). It was assumed that the level of CYP3A4 was immediately restored to steady state levels at renewal. The system allowed a scaling of the resolution of the enterocyte compartment, where the number of enterocytes could be altered based on *e.g.* computational time (Equation 6.8 and Figure 6.1).

$$f(t, A_{Ent-Lifespan,N}, A_{CYP3A-GI,N}) = \begin{cases} A_{Ent-Lifespan,i} = 0, A_{CYP3A-GI,i} = A_{CYP3A-GI,SS} & \text{if } A_{Ent-Lifespan,i} \geq 1 \\ A_{Ent-Lifespan,i}(t), A_{CYP3A-GI,i}(t) & \text{else} \end{cases}$$

Equation 6.8. NEWE model (3): Time to event function.

The developed NEWE model was further coupled to a minimal PBPK absorption model, describing the amount of inhibitor as it was administered into the gut lumen ($A_{I,lumen}$), the rate of absorption into the enterocytes (k_a) and the rate of elimination via small intestinal transit (k_{sit}), where the cumulative elimination was equal to $1 - f_a$ (the fraction of administered drug that is absorbed through the gut wall) (Equation 6.9 and Figure 6.1).

$$\frac{dI_{lumen}}{dt} = -A_{I,lumen} \cdot (k_a + k_{sit})$$

Equation 6.9. NEWE model (4): Inhibitor concentration in gut lumen.

The inhibitory concentration in the enterocyte (I_{ent}) was dependent on the volume of the enterocyte tissue (V_{ent}), rate of absorption from the small intestine ($k_a \cdot A_{I,lumen}$) and further clearance through the villous blood flow (Q_{villi}) and an unbound inhibitory clearance ($CLu_{int,gut}$) dependent on the fraction of unbound inhibitor in the enterocytes (fu_{gut}) (Equation 6.10).

$$V_{ent} \cdot \frac{dI_{ent}}{dt} = A_{I,lumen} \cdot k_a - I_{ent} \cdot (Q_{villi} + CLu_{int,gut} \cdot fu_{gut})$$

Equation 6.10. NEWE model (5): Inhibitor concentration in the enterocytes.

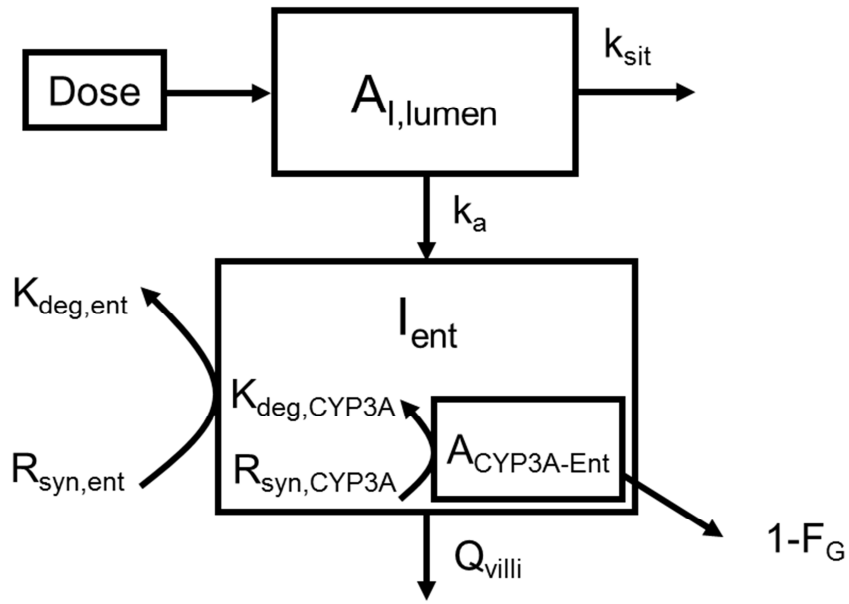


Figure 6.1. Model schematics of the nested enzyme-within-enterocyte model, Amount of inhibitor in the gut lumen ($A_{I,lumen}$) and concentration of inhibitor in the enterocytes (I_{ent}). Indicated rates and blood flows include: absorption rate constant (k_a) and small intestinal transit rate (k_{sit}), villous blood flow (Q_{villi}), portal vein blood flow (Q_{pv}), hepatic artery blood flow (Q_{ha}), and hepatic blood flow (Q_{hep}). $R_{syn,ent}$ and $k_{deg,ent}$ are the production and degradation rate of the enterocytes respectively. $R_{syn,CYP3A}$ $K_{deg,CYP3A}$ indicate the synthesis and degradation rate of CYP3A4 in the small intestine.

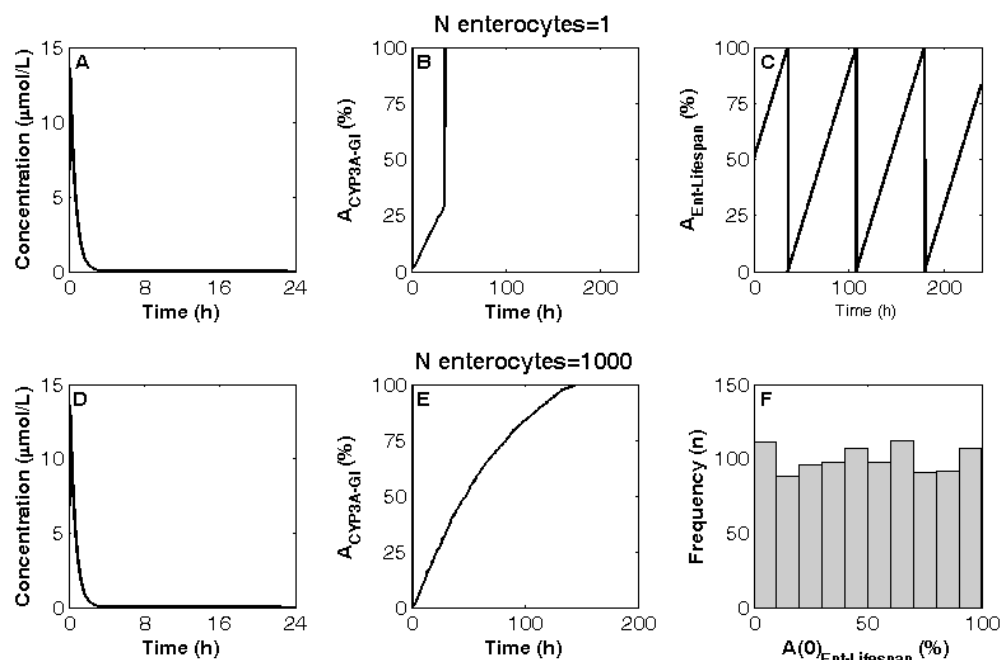


Figure 6.2. Conceptual simulation of an enterocyte ($n=1$) utilising the proposed model, displaying **A:** Inhibitor concentration in the enterocyte tissue, **B:** Relative activity of CYP3A4 in the small intestine ($A_{\text{CYP3A-GI}}$) over time following mechanism-based inhibition, **C:** Enterocyte life progression and regeneration over time. Conceptual simulations of $n=1000$ enterocytes **D:** Inhibitor concentration in the enterocyte tissue, **E:** $A_{\text{CYP3A-GI}}$ following mechanism-based inhibition, **F:** Distribution of initial starting points of the enterocyte population life progression ($A(t=0)_{\text{Ent-Lifespan}}$).

6.4.2 Exploratory sensitivity analysis - study design

Parameter ranges utilised for the simulation-based exploratory sensitivity analysis were based on observed data, where the inhibitor specific parameters were based on 37 compounds, displaying a geometric mean K_{Iu} of 5.15 and a 95% confidence interval (CI95) of 0.14-119.50 μM , ranging from 0.06 to 1640 μM . K_{inact} displayed a geometric mean of 7.18 h^{-1} (CI95: 1.61-34.26, range: 1.02-120). Gastrointestinal $k_{\text{deg,ent-CYP3A4}}$ was based on data from 13 studies (n samples=121), ranging from 0.005-0.069 h^{-1} (Figure 6.3) (Zhou *et al.*, 2005; Yang *et al.*, 2008). Static parameters k_a and dose were set to 1.5 h^{-1} and 200 μmol respectively based on the 17th WHO model list of Essential Medicines (n drugs=74; see Appendix 8.5) (WHO, 2011).

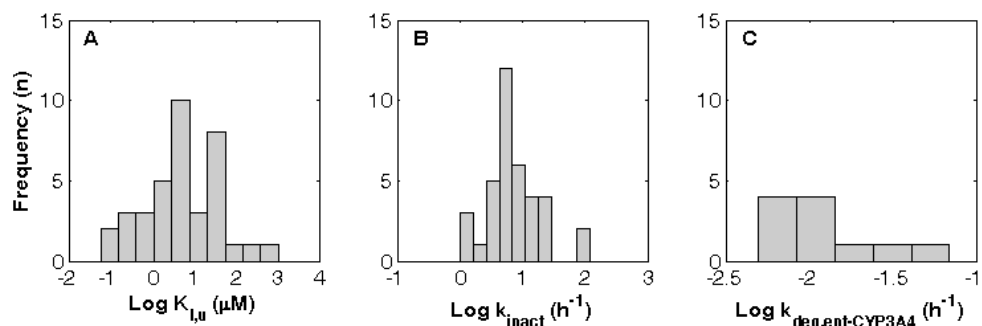


Figure 6.3. Observed distribution of the frequency of the reported inhibitor specific parameters, including: The concentration that produces half the maximal rate of inactivation ($K_{I,u}$ [μM]) maximal rate of inactivation (k_{inact} [h^{-1}]) and turnover rate of small intestinal CYP3A4 ($k_{\text{deg,Ent-CYP3A4}}$ [h^{-1}]).

The sensitivity analysis study design included six values of $k_{\text{deg,Ent}}$ (0.083, 0.042, 0.014, 0.007 0.006 and 0.003 h^{-1}), six values of $k_{\text{deg,CYP3A}}$ (0.001, 0.003, 0.007, 0.01, 0.03 and 0.07 h^{-1}), five values of $K_{I,u}$ (0.01, 0.1, 5, 100 and 2000 μM) and three values of k_{inact} (1, 10 and 150 h^{-1}) resulting in a total of 630 simulations (Figure 6.4).

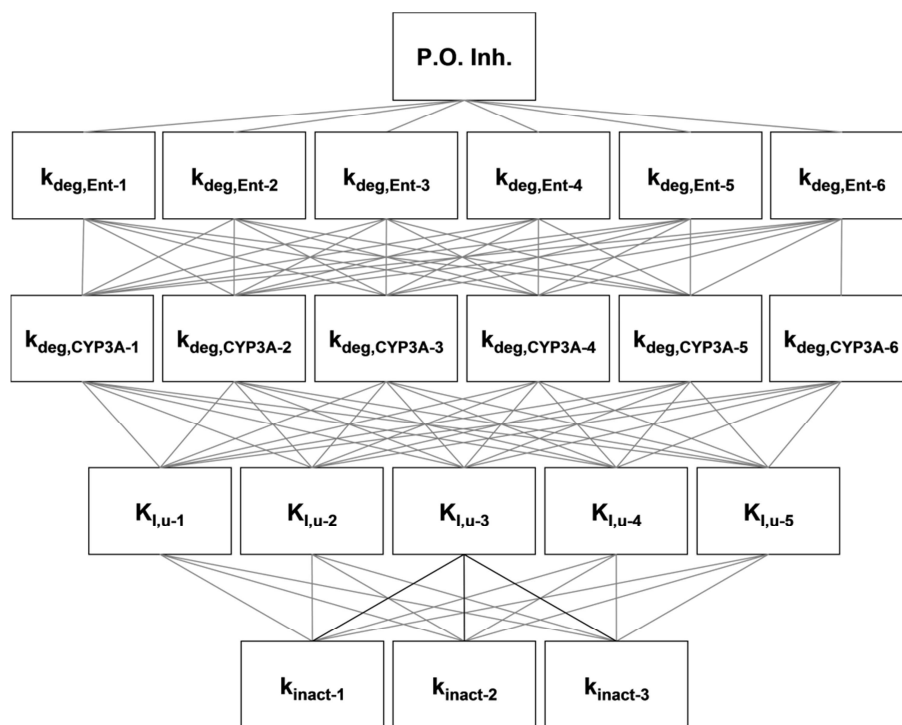


Figure 6.4. Study design of exploratory simulation assessment of an orally administered single dose of a mechanism-based inhibitor (p.o. Inh.), introducing systematic variation to four parameter levels, including: Life progression rate of enterocytes ($k_{deg,Ent-(1-7)}$), degradation rate of enterocytic CYP3A4 ($k_{deg,CYP3A-(1-6)}$), ($K_{I,u-(1-5)}$) and ($k_{inact-(1-3)}$) resulting in a total of 630 simulations using a resolution of $n=1,000$ enterocytes.

6.4.3 Exploratory sensitivity analysis - results

Examining the simulated relative activity of CYP3A4 in the gastrointestinal tract over 24h following MBI relative to the standard model scenario only taking changes to $k_{deg,CYP3A}$ into account ($A_{Ent-n/0,0-24h} [\%]; k_{deg,Ent}=0 h^{-1}$), the CYP3A4 activity was either increased or unaltered using the NEWE model in the majority simulated scenarios. Considering $A_{Ent-n/0,0-24h}$ as a function of $k_{deg,Ent}$ and $k_{deg,CYP3A4}$ the most extensive increase in $A_{CYP3A4,0-24h}$ was observed at a maximum $k_{deg,Ent}$ and $k_{deg,CYP3A4}$ of 0.08 and $0.07 h^{-1}$ respectively, displaying a $A_{Ent-n/0,0-24h}$ ranging from 100.0 to 7,295% dependent on the inhibitor specific parameters ($K_{I,u}$ and k_{inact} ; Figure 6.5).

Increasing inhibitor specific $K_{I,u}$ generally resulted in a reduction in $A_{Ent-n/0,0-24h}$, where the increase in relative CYP3A4 activity following MBI varied from 100 to 156.4% at a

midrange $K_{I,u}$ (5 μM) and a low k_{inact} (1 h^{-1}). A reduction in $K_{I,u}$ to 0.1 μM led to an increase in relative CYP3A4 activity, where $A_{\text{Ent-n/0,0-24h}}$ varied between 100 and 1,063.6%. Discrepancies in CYP3A4 activity between the two models were less sensitive to alterations in $k_{\text{deg,Ent}}$ and $k_{\text{deg,CYP3A}}$ at a $K_{I,u}$ of 2000 μM , displaying $A_{\text{Ent-n/0,0-24h}}$ between 100-100.3% (Figure 6.5).

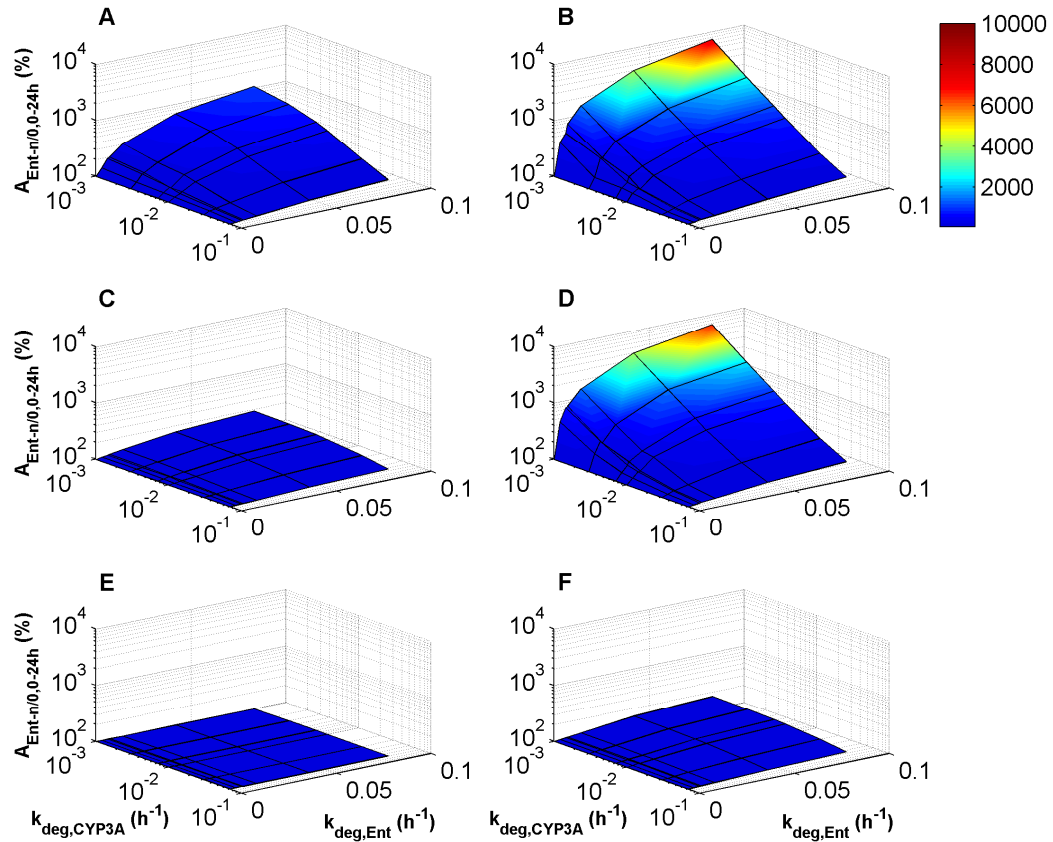


Figure 6.5. Simulated relative activity of CYP3A4 in the gastrointestinal tract over 24h following mechanism-based inhibition relative to the standard model scenario only taking changes to CYP3A4 degradation rate ($k_{\text{deg,CYP3A}}$) into account (enterocyte degradation rate [$k_{\text{deg,Ent}}=0 \text{ h}^{-1}$; $A_{\text{CYP3A4,0-24h}} k_{\text{deg,Ent-n/0}}$ [%]]) in relation to $k_{\text{deg,CYP3A}}$ (h^{-1}) and $k_{\text{deg,Ent-n/0}}$ (h^{-1}), varying the maximal rate of enzyme inactivation (k_{inact} [h^{-1}]) and the inhibitor concentration that produces half of the maximal rate of inactivation ($K_{I,u}$ [μM]) **A:** $K_{I,u}=0.01 \mu\text{M}$ and $k_{\text{inact}}=1 \text{ h}^{-1}$, **B:** $K_{I,u}=0.01 \mu\text{M}$ and $k_{\text{inact}}=150 \text{ h}^{-1}$, **C:** $K_{I,u}=5 \mu\text{M}$ and $k_{\text{inact}}=1 \text{ h}^{-1}$, **D:** $K_{I,u}=5 \mu\text{M}$ and $k_{\text{inact}}=150 \text{ h}^{-1}$, **E:** $K_{I,u}=2000 \mu\text{M}$ and $k_{\text{inact}}=1 \text{ h}^{-1}$, and **F:** $K_{I,u}=2000 \mu\text{M}$ and $k_{\text{inact}}=150 \text{ h}^{-1}$.

An increase in k_{inact} generally lead to an increase $A_{\text{Ent-n/0,0-24h}}$. At a high k_{inact} (150 h^{-1}) the increase in $A_{\text{Ent-n/0,0-24h}}$ became more apparent, resulting in an increase in the relative CYP3A4 activity from 100.0 to 7,295% at a low $K_{\text{I,u}}$ ($0.1 \text{ }\mu\text{M}$), whereas $A_{\text{Ent-n/0,0-24h}}$ ranged between 100 and 169% at a high $K_{\text{I,u}}$ ($2000 \text{ }\mu\text{M}$) (Figure 6.5).

Examining the simulated relative activity of CYP3A4 in the gastrointestinal tract over 240 h following MBI as compared to impact of MBI on A_{CYP3A4} using the conventional model predictions, $A_{\text{Ent-n/0,0-24h}}$, resulted in a less pronounced sensitivity to alterations in $k_{\text{deg,Ent}}$ and $k_{\text{deg,CYP3A4}}$ as compared to the activity up to 24h, displaying a maximum simulated $A_{\text{Ent-n/0,0-24h}}$ of 903% following MBI up to 240h at a $K_{\text{I,u}}$ of $0.01 \text{ }\mu\text{M}$, k_{inact} 150 h^{-1} , $k_{\text{deg,Ent}}$ of 0.003 h^{-1} and $k_{\text{deg,CYP3A}}$ of 0.001 h^{-1} (Figure 6.6).

Considering the activity of small intestinal CYP3A4 following MBI, relative to activity at a $k_{\text{deg,Ent}}$ of zero, as a function of $K_{\text{I,u}}$ and $k_{\text{deg,CYP3A}}$ and varying $k_{\text{deg,Ent}}$ and k_{inact} , $A_{\text{Ent-n/0,0-24h}}$ displayed an apparent non-linear relationship in the lower range of $K_{\text{I,u}}$'s and a low to medium k_{inact} ($1\text{-}10 \text{ h}^{-1}$). Further, the $A_{\text{Ent-n/0,0-24h}}$ in general displayed lower sensitivity to $K_{\text{I,u}}$ at a high $k_{\text{deg,CYP3A}}$. $A_{\text{Ent-n/0,0-24h}}$ varied from 100 to 1,064% at a high $k_{\text{deg,Ent}}$ (0.083 h^{-1}), whereas a low $k_{\text{deg,Ent}}$ (0.006 h^{-1}), resulted in a lower sensitivity to $K_{\text{I,u}}$ with a $A_{\text{Ent-n/0,0-24h}}$ ranging from 101 to 7295% (Figure 6.7 A, B, D, E, G and H).

At a high k_{inact} (150 h^{-1}) $A_{\text{Ent-n/0,0-24h}}$ displayed a more linear relation to $K_{\text{I,u}}$ with a less apparent sensitivity to $K_{\text{I,u}}$ at a high $k_{\text{deg,CYP3A}}$. $A_{\text{Ent-n/0,0-24h}}$ displayed less sensitivity to $k_{\text{deg,CYP3A}}$ and $K_{\text{I,u}}$ at a high $k_{\text{deg,Ent}}$ (0.083 h^{-1}) ranging from 103 to 903% at a low $k_{\text{deg,Ent}}$ (0.006 h^{-1}) and 100 to 382% at a high $k_{\text{deg,Ent}}$ (0.083 h^{-1}) (Figure 6.7 C, F and I).

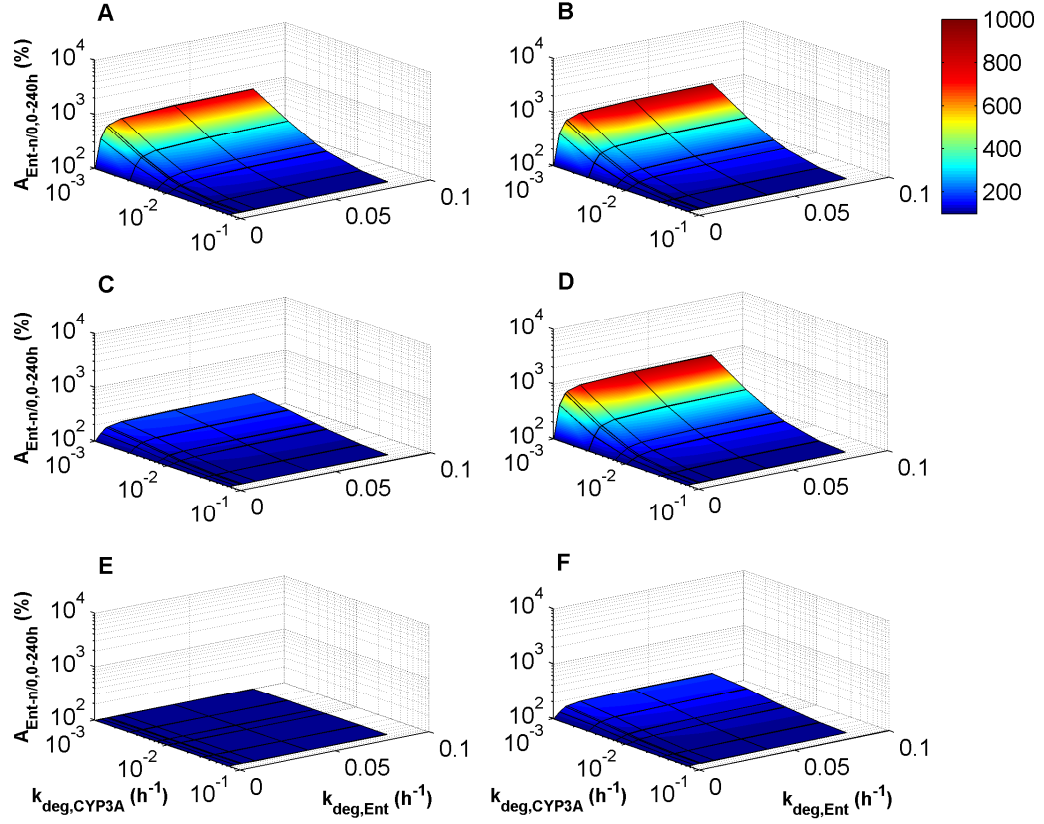


Figure 6.6. Simulated activity of CYP3A4 in the gastrointestinal tract over 240h following mechanism-based inhibition relative to the standard model scenario only taking changes to CYP3A4 degradation rate ($k_{\text{deg,CYP3A}}$) into account (enterocyte degradation rate [$k_{\text{deg,Ent}}$]=0 h^{-1} ; $A_{\text{Ent-n/0,0-24h}}$ [%]) in relation to $k_{\text{deg,CYP3A}}$ (h^{-1}) and $k_{\text{deg,Ent}}$ (h^{-1}), varying the maximal rate of enzyme inactivation (k_{inact} [h^{-1}]) and the inhibitor concentration that produces half of the maximal rate of inactivation ($K_{\text{I,u}}$ [μM]) **A:** $K_{\text{I,u}}$ =0.01 μM and k_{inact} =1 h^{-1} , **B:** $K_{\text{I,u}}$ =0.01 μM and k_{inact} =150 h^{-1} , **C:** $K_{\text{I,u}}$ =5 μM and k_{inact} =1 h^{-1} , **D:** $K_{\text{I,u}}$ =5 μM and k_{inact} =150 h^{-1} , **E:** $K_{\text{I,u}}$ =2000 μM and k_{inact} =1 h^{-1} , and **F:** $K_{\text{I,u}}$ =2000 μM and k_{inact} =150 h^{-1} .

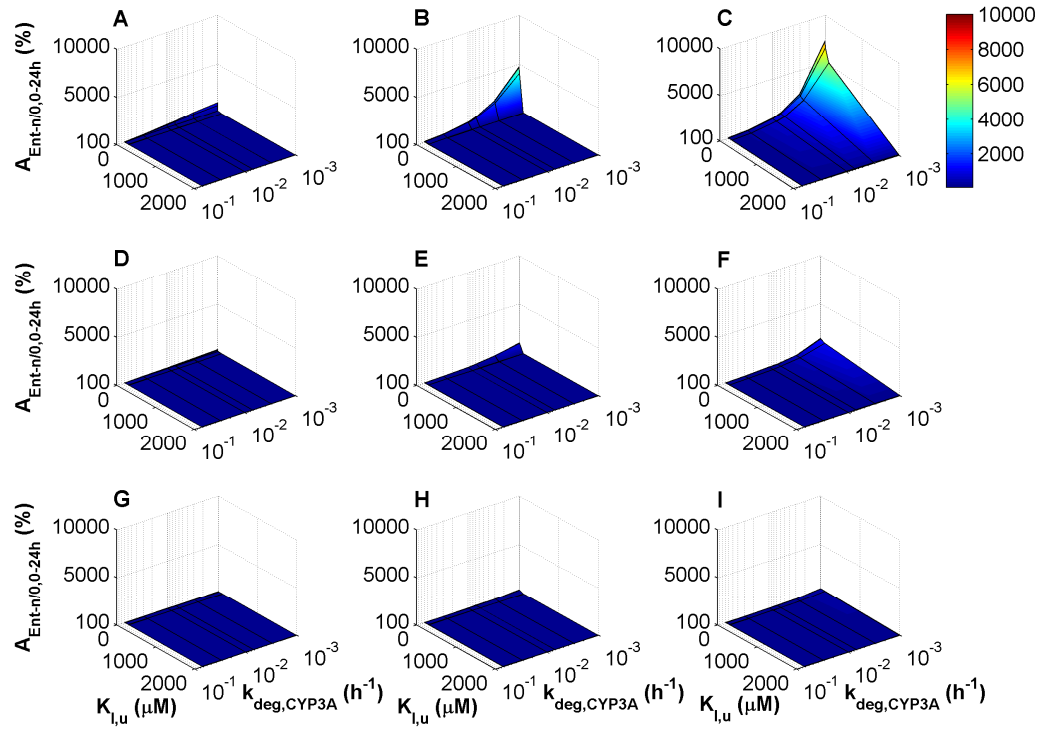


Figure 6.7. Simulated activity of CYP3A4 in the gastrointestinal tract over 24h following mechanism-based inhibition relative to the standard model scenario only taking changes to CYP3A4 degradation rate ($k_{deg,CYP3A}$) into account (enterocyte degradation rate $[k_{deg,Ent}]=0 \text{ h}^{-1}$; $A_{Ent-n/0,0-240h} [\%]$) in relation to $K_{I,u}$ (the inhibitor concentration that produces half of the maximal rate of inactivation $[\mu\text{M}]$) and $k_{deg,CYP3A}$ (h^{-1}), varying $k_{deg,Ent}$ and k_{inact} (maximal rate of enzyme inactivation) **A:** $k_{deg,Ent}=0.083 \text{ h}^{-1}$ and $k_{inact}=1 \text{ h}^{-1}$, **B:** $k_{deg,Ent}=0.007 \text{ h}^{-1}$ and $k_{inact}=10 \text{ h}^{-1}$, **C:** $k_{deg,Ent}=0.006 \text{ h}^{-1}$ and $k_{inact}=150 \text{ h}^{-1}$, **D:** $k_{deg,Ent}=0.083 \text{ h}^{-1}$ and $k_{inact}=1 \text{ h}^{-1}$, **E:** $k_{deg,Ent}=0.007 \text{ h}^{-1}$ and $k_{inact}=10 \text{ h}^{-1}$, **F:** $k_{deg,Ent}=0.006 \text{ h}^{-1}$ and $k_{inact}=50 \text{ h}^{-1}$, **G:** $k_{deg,Ent}=0.083 \text{ h}^{-1}$ and $k_{inact}=1 \text{ h}^{-1}$, **H:** $k_{deg,Ent}=0.007 \text{ h}^{-1}$ and $k_{inact}=10 \text{ h}^{-1}$, and **I:** $k_{deg,Ent}=0.006 \text{ h}^{-1}$ and $k_{inact}=150 \text{ h}^{-1}$.

Considering $A_{Ent-n/0,0-24h}$ as a function of $K_{I,u}$ and k_{inact} , varying $k_{deg,Ent}$ and $k_{deg,CYP3A}$, $A_{Ent-n/0,0-240h}$ displayed an apparent low sensitivity to $K_{I,u}$ and k_{inact} . At a low $k_{deg,CYP3A}$ (0.001 h^{-1}), with a $A_{Ent-n/0,0-24h}$ varying from 135.5 to 999% at a $k_{deg,Ent}$ varying from 0.014 to 0.003 h^{-1} . At a high $k_{deg,CYP3A}$ (0.07 h^{-1}) $A_{Ent-n/0,0-24h}$ displayed a low sensitivity varying from 101.46 to 113.43 % at a $k_{deg,Ent}$ varying from 0.014 to 0.003 h^{-1} (Figure 6.8).

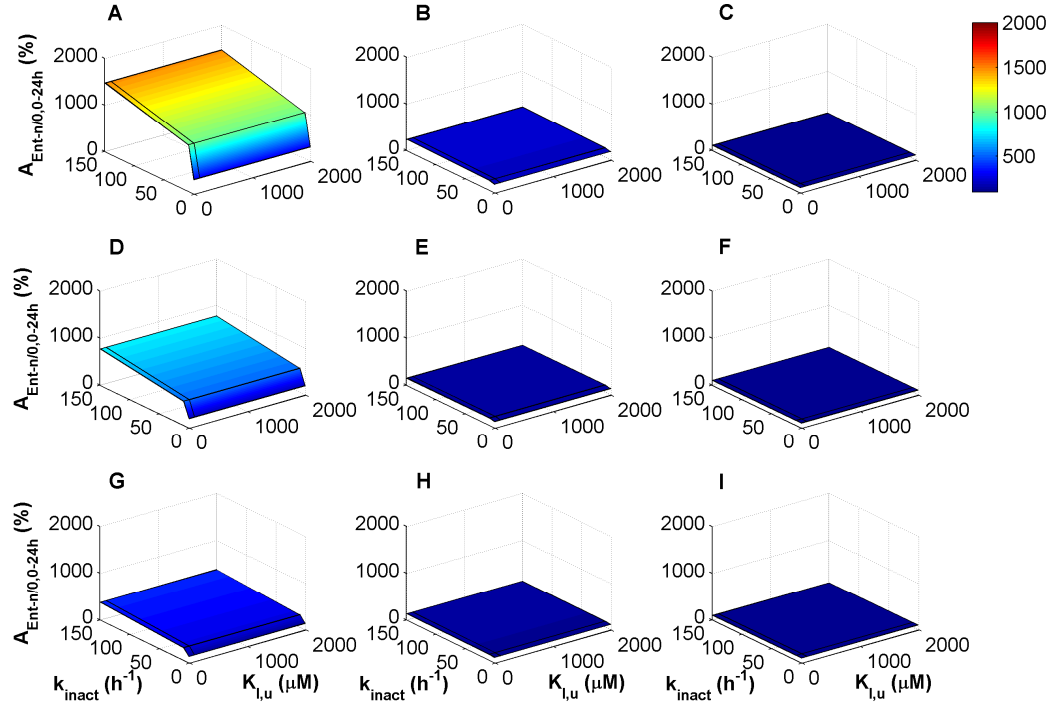


Figure 6.8. Simulated relative activity of CYP3A4 in the gastrointestinal tract over 240h following mechanism-based inhibition relative to the standard model scenario only taking changes to CYP3A4 degradation rate ($k_{deg,CYP3A}$) into account (enterocyte degradation rate $[k_{deg,Ent}]=0 \text{ h}^{-1}$; $A_{Ent-n/0,0-240h} [\%]$) in relation to $K_{I,u}$ (the inhibitor concentration that produces half of the maximal rate of inactivation $[\mu\text{M}]$) and k_{inact} (the maximal rate of enzyme inactivation $[\text{h}^{-1}]$), varying $k_{deg,Ent}$ and $k_{deg,CYP3A}$ **A:** $k_{deg,Ent}=0.0139 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.001 \text{ h}^{-1}$, **B:** $k_{deg,Ent}=0.0139 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.01 \text{ h}^{-1}$, **C:** $k_{deg,Ent}=0.0139 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.07 \text{ h}^{-1}$, **D:** $k_{deg,Ent}=0.007 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.001 \text{ h}^{-1}$, **E:** $k_{deg,Ent}=0.007 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.01 \text{ h}^{-1}$, **F:** $k_{deg,Ent}=0.007 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.07 \text{ h}^{-1}$, **G:** $k_{deg,Ent}=0.003 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.001 \text{ h}^{-1}$, **H:** $k_{deg,Ent}=0.003 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.01 \text{ h}^{-1}$, **I:** $k_{deg,Ent}=0.003 \text{ h}^{-1}$ and $k_{deg,CYP3A}=0.07 \text{ h}^{-1}$.

Simulations utilising the NEWE model at $k_{deg,Ent}$ of 0.013 h^{-1} , based on current study, and $k_{deg,CYP3A}$ of 0.027 h^{-1} ($t_{1/2}=26 \text{ h}$) based *in vitro* data estimated by Yang, and co-workers (2008), was compared to the conventional model ($k_{deg,Ent}=0 \text{ h}^{-1}$) using a $k_{deg,CYP3A}$ of 0.03 h^{-1} based on the recovery time of intestinal CYP3A4 estimated by Yang, and co-workers (Yang *et al.*, 2008).

In agreement with the sensitivity analysis, a higher activity of CYP3A was displayed utilising the NEWE model for inhibitors exhibiting a high k_{inact} and a low $K_{\text{I,u}}$, with a $A_{\text{Ent-n/0,0-240h}}$ varying from 100.04% at a $K_{\text{I,u}}$ of 2,000 μM and k_{inact} of 1 h^{-1} , to 647.26% at $K_{\text{I,u}}$ of 0.01 μM and a k_{inact} of 150 h^{-1} (Figure 6.9).

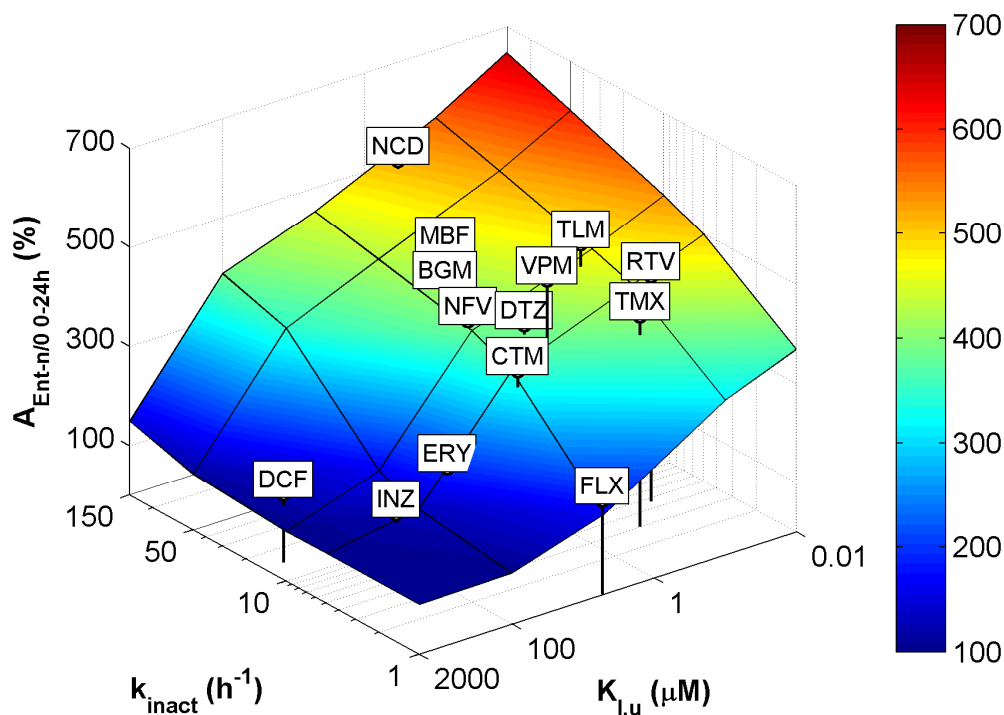


Figure 6.9. Simulated relative activity of CYP3A4 in the gastrointestinal tract over 24h following single dose mechanism-based inhibition using the nested enzyme-within-enterocyte (NEWE) model relative to the conventional model scenario ($A_{\text{Ent-n/0,0-24h}}$ [%]) in relation to $K_{\text{I,u}}$ (the inhibitor concentration that produces half of the maximal rate of inactivation [μM]) and k_{inact} (the maximal rate of enzyme inactivation [h^{-1}]). FLX=fluoxetine, TMX=tamoxifen, CTM=clarithromycin, RTV=ritonavir, ERM=erythromycin, INZ=isoniazid, VPM=verapamil, DTZ=diltiazem, TLM=troleandomycin, NFV=nelfinavir, DCF=diclofenac, BGM=bergamottin, MBF=mibefradil and NCD=nicardipine.

Comparing simulations of multiple dose inhibition, once daily for three days, using the NEWE model and conventional modelling approach the NEWE model displayed higher CYP3A activity as compared to the conventional modelling approach, albeit to a lesser extent as compared to single dose simulations. $A_{\text{Ent-n/0,48-72h}}$ varied from 100%, at a $K_{\text{I,u}}$

of 2000 μM and a k_{inact} of 1 h^{-1} , to 209% at a $K_{\text{I,u}}$ of $0.1 \mu\text{M}$ and a k_{inact} of 1 h^{-1} (Figure 6.10).

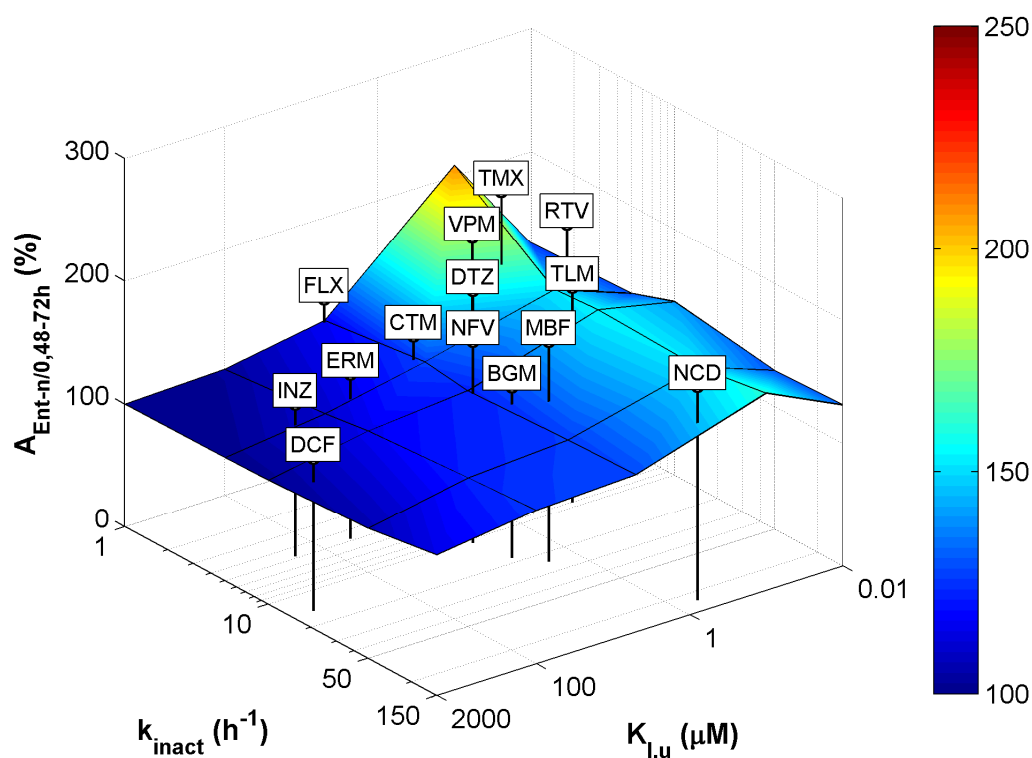


Figure 6.10. Simulated relative activity of CYP3A4 in the gastrointestinal tract over 24h following multiple dosing mechanism-based inhibition using the nested enzyme-within-enterocyte (NEWE) model relative to the conventional model scenario ($A_{\text{Ent-n/0,48-72h}} [\%]$) in relation to $K_{\text{I,u}}$ (the inhibitor concentration that produces half of the maximal rate of inactivation [μM]) and k_{inact} (the maximal rate of enzyme inactivation [h^{-1}]). FLX=fluoxetine, TMX=tamoxifen, CTM=clarithromycin, RTV=ritonavir, ERM=erythromycin, INZ=isoniazid, VPM=verapamil, DTZ=diltiazem, TLM=troleandomycin, NFV=nelfinavir, DCF=diclofenac, BGM=bergamottin, MBF=mibefradil and NCD=nicardipine.

6.5 Discussion

Overall, the developed NEWE model produced a higher small intestinal CYP3A4 activity following mechanism-based inhibition as compared to the conventional PBPK modelling approach ($k_{\text{deg,Ent}}=0 \text{ h}^{-1}$). The NEWE model displayed a higher level of CYP3A4 activity following MBI as a consequence of an increase in $k_{\text{deg,Ent}}$ and $k_{\text{deg,CYP3A}}$. Inhibitors displaying a low $K_{\text{I,u}}$ or high k_{inact} were more likely to give rise to a lower level of inhibition, where a combination of a low $K_{\text{I,u}}$ and a high k_{inact} led to the lowest level of inhibition, using the NEWE model as compared to the conventional model (Figure 6.5-6.10).

Comparing the outcome of the NEWE model on intestinal CYP3A4 activity using observed data of $k_{\text{deg,Ent}}$ and $k_{\text{deg,CYP3A}}$ as compared to the hybrid parameter $k_{\text{deg,CYP3A}}$ in the conventional model, indicated the NEWE model to display a lower degree of inhibition for a number of mechanism-based inhibitors. The increase in intestinal CYP3A4 activity was further apparent for inhibitors where over-predictions have been observed utilising a conventional modelling approach, including fluoxetine ($K_{\text{I,u}}=5.19 \mu\text{M}$, $k_{\text{inact}}=1.02 \text{ h}^{-1}$) and mibefradil ($K_{\text{I,u}}=2.23 \mu\text{M}$, $k_{\text{inact}}=24 \text{ h}^{-1}$), displaying approximately 13% and 31% higher activity of intestinal CYP3A4 respectively following MBI (Figure 6.9).

The data utilised for observed values of $k_{\text{deg,Ent}}$ and $k_{\text{deg,CYP3A}}$ and the surrogate parameter of $k_{\text{deg,CYP3A}}$ were however suffering from a high degree of uncertainty where lack of variance in reported data limited the simulation to the use of arithmetic mean values. The enzyme turnover data was based on human *in vitro* hepatocyte assays, where it is questionable how this translates into small intestinal CYP3A4 turnover *in vivo* (Yang *et al.*, 2008). The surrogate parameter of $k_{\text{deg,Ent}}$ and $k_{\text{deg,CYP3A}}$ was based on the rate of recovery of grapefruit juice studies in man, known to display a high variability in the level of inhibition depending on the volume grapefruit juice consumed and its concentration of inhibitory constituents, displaying a large variability between batches. It has further been observed *in vivo* that the inhibitory constituents are both mechanism-based and reversible inhibitors, thus leading to a potential overestimation in $k_{\text{deg,CYP3A}}$ based on grapefruit juice data (Paine *et al.*, 2004; Uesawa *et al.*, 2011). Further, the estimate of $k_{\text{deg,Ent}}$ was subject to limitations in sample size, where a the majority of the data was based on colorectal and gastric epithelium turnover data.

Method limitations for measuring $k_{\text{deg,Ent}}$ also limited the human data to mainly consist of cancer patients where discrepancies may exist as compared to a healthy population.

In conventional PBPK approaches to modelling MBI the enzyme turnover rate is modelled as a first-order rate (Rowland Yeo *et al.*, 2010); whereas the gastrointestinal epithelial cell population conforms to a uniform distribution where the turnover is most likely to follow a zero-order rate or be of a sequential nature, where for example the distribution of DNA synthesising cells in the small intestine has been indicated to conform to a random or asynchronous distribution (Bell *et al.*, 1967; van Leeuwen *et al.*, 2009). As a consequence the NEWE model may improve the prediction of not only the extent and timeframe of MBI but also describing the time profile at which recovery of active enzyme occurs in the small intestine.

A more physiological modelling approach may further allow the prediction of DDIs in special subpopulations where small intestinal mucosal structure, enzyme or enterocyte turnover are altered. Alteration to the renewal of the small intestinal epithelium has been observed for a number of disease conditions in man, including: Coeliac disease patients, patients subject to small intestinal resection, patients subject to radiation therapy and untreated patients with pernicious anaemia or vitamin B₁₂ and folate deficiency (Winawer *et al.*, 1965; Trier and Browning, 1966; Foroozan and Trier, 1967; Weinstein *et al.*, 1969). Certain drugs may also affect the turnover of the enterocytes, where altered small intestinal epithelial cell renewal has been observed following treatment with antibiotics, cancer chemotherapy, colchicine and methotrexate (Trier, 1962; Race *et al.*, 1970; Weinstein, 1974).

In addition to alterations of the enterocyte renewal in disease populations, pre-clinical data imply alterations in the turnover as a consequence of age e.g., in lambs and piglets, an increase in epithelial cell turnover time was observed as a consequence of postnatal adaptation of the small intestine following birth (Attaix and Meslin, 1991).

Contrasting evidence exist regarding the regional difference in enterocyte turnover along the small intestine. In neonatal pig the distal small intestine displayed a slower turnover as compared to the proximal small intestine using bromodeoxyuridine labeling assay; whereas regional differences in enterocyte turnover between the small intestine

and colon have been observed in rat, although differences between duodenum, jejunum and ileum were minimal (Bertalanffy and Lau, 1962; Fan *et al.*, 2001). In the previous study, analysis of human data on gastrointestinal epithelial turnover identified the colorectal cell renewal to be slower as compared to the stomach, whereas data from the small intestinal regions were too sparse in order to capture any regional differences (Figure 5.5).

The development of the NEWE model was subject to a number of assumptions where the modelling approach did not consider the maturation of enterocytes, metabolic and absorptive capability or any regional differences in turnover, albeit the collated information of $k_{deg,Ent}$ did not support this. The sensitivity analysis was limited to altering a restricted number of drug specific parameters, where k_a , dose and the clearance of the inhibitor was kept at a constant level which only satisfies hypothetical scenarios of MBI. The developed model therefore requires validation against clinical MBI data in order to determine if improvements are made in the prediction of DDIs. Due to the sparse data on enzyme and enterocyte turnover the level at which the small intestinal activity of CYP3A4 differs may differ in reality due to the uncertainty in the estimates of $k_{deg,Ent}$ and $k_{deg,CYP3A}$, although the discrepancy between the two models should remain as indicated by the sensitivity analysis where the overall trend was that the NEWE model produced equal or higher level of intestinal CYP3A4 activity.

The developed NEWE model is, to our knowledge, the first PBPK model to consider the nesting and hierarchy of the enzyme and enterocyte turnover in the small intestine. The model has the potential to improve on predictions of mechanism-based inhibition where overpredictions have been observed. The utilisation of a more physiological description of small intestinal enzyme and cell dynamics following DDIs has the potential for further application on a number of subpopulations and disease states where the enzyme or enterocyte turnover may be altered.

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6.7 References

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Chapter 7: Discussion and conclusions

Chapter 7: Discussion and conclusions

In this thesis, a systems pharmacology approach utilising physiologically-based pharmacokinetic modelling and simulation coupled to *in vitro-in vivo* extrapolation was utilised to model oral drug bioavailability with a particular interest in the gastrointestinal component. Two cases were investigated where $f_a \cdot F_G$ plays a potentially important role in the prediction of systemic exposure, thus allowing the exploration of the interplay between oral drug absorption and metabolism in the gut-wall. Examined cases were PBPK M&S of trends in oral drug exposure in a morbidly obese patient population subject to bariatric surgery and the development and assessment of a nested enzyme-within-enterocyte model in order to improve the mechanistic description of mechanism-based inhibition of gut wall metabolism facilitated by CYP3A.

7.1 PBPK M&S of oral drug bioavailability post bariatric surgery

Post bariatric surgery PBPK models were developed through a systematic approach including the identification of population dependent intrinsic factors, characterisation of systems parameters, model development and implementation based on the mechanistic model for oral drug bioavailability, the ADAM model. Assessment of the perturbed model was carried out using sensitivity analysis and validation against clinical data.

The outcome of the validation exercise of post bariatric surgery PBPK models was to some extent reflective how well characterised the systems parameters of intrinsic factors were, where the most well-characterised post bariatric surgery model, post Roux-en-Y gastric bypass, was highly predictive of clinical outcomes of oral drug exposure of atorvastatin acid and cyclosporine, whereas oral drug exposure of atorvastatin acid following BPD-DS was underpredicted using the standard model including all known physiological changes. Additional validation occurred prospectively through generation of clinical data of omeprazole and midazolam pre to post RYGB by Tandra, and co-workers. The study found omeprazole to display a minimal discrepancy post RYGB as compared to controls, whereas midazolam displayed a minor increase in exposure post RYGB as compared to controls. This was consistent with simulations carried out during the model assessment and application (Figure 3.9, Figure 7.1 and Figure 8.6) (Darwich *et al.*, 2012b; Tandra *et al.*, 2013).

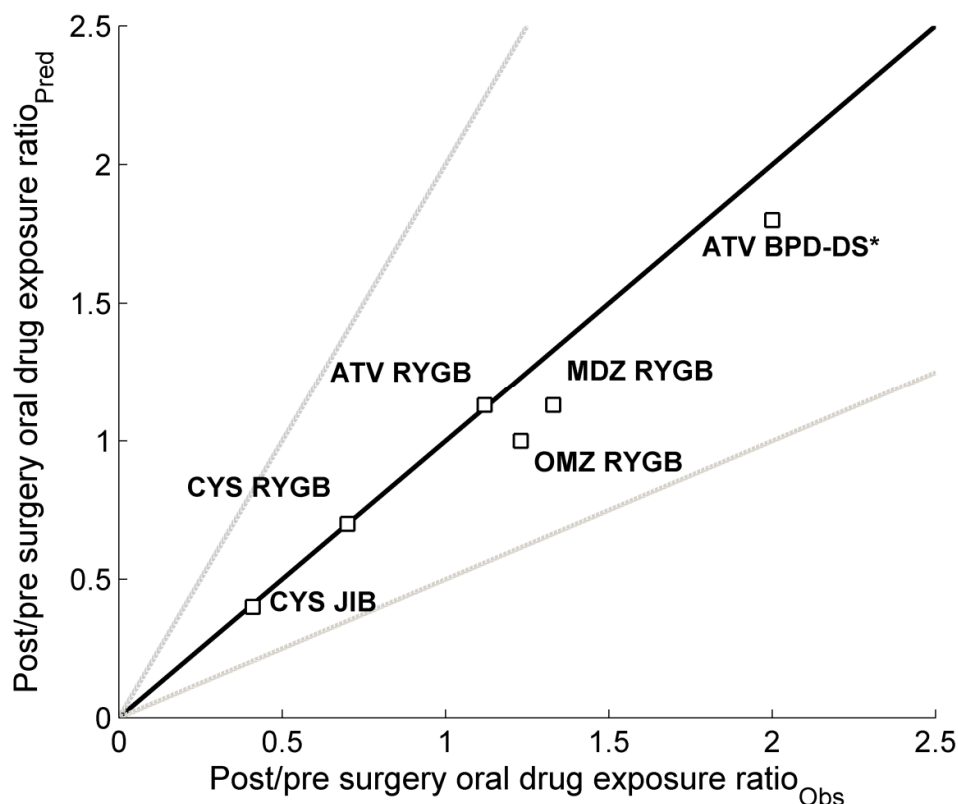


Figure 7.1. Mean predicted (Pred) versus observed (Obs) post/pre surgery AUC ratios for cyclosporine (CYS), atorvastatin acid (ATV), omeprazole (OMZ) and midazolam (MDZ) following Roux-en-Y gastric bypass (RYGB) at a small intestinal transit (SIT) time of 3.0 h, jejunioileal bypass (JIB SIT=0.4 h) and biliopancreatic diversion with duodenal switch (BPD-DS* SIT=4.2 h) in relation to the line of unity and two-fold within observed data (Chenhsu *et al.*, 2003; Skottheim *et al.*, 2009; Skottheim *et al.*, 2010; Darwich *et al.*, 2012b; Tandra *et al.*, 2013; Darwich *et al.*, 2013).

The discrepancy between observed and simulated exposure of atorvastatin acid pre to post BPD-DS could be anticipated as the BPD-DS model was populated with relatively uninformative systems parameters of small intestinal transit and biliary excretion, it was further speculated that the surgical procedure may produce unanticipated physiological outcomes due to its relative invasiveness as compared to RYGB and SG. The PBPK M&S approach did however have the advantage of allowing exploratory sensitivity analysis, where a prediction of small intestinal transit based on peptide YY-mouth-to-

caecum transit recovered the observed exposure albeit underpredicting observed C_{\max} and t_{\max} , the same was true for altering villous blood flow.

Hendriks highlighted that for the publication of negative results in M&S to be justified necessary considerations have to be made regarding a model's credibility where evaluation of a model's credibility becomes increasingly difficult as PBPK models become more complex. This holds true for both positive and negative prediction outcomes. Hendriks further argued that necessary steps should be taken to articulate how the negative finding may inform scientific and hypotheses generation (Hendriks, 2013).

The utilised ADAM model and its predecessors have been applied extensively in the past (Jamei *et al.*, 2009). In the publication by Darwich, and co-workers, it was however made clear that physiological data was lacking for crucial systems parameters following BPD-DS (Darwich *et al.*, 2013). The sensitivity analysis of atorvastatin acid exposure following BPD-DS provided a potential scientific rationale for the observed increase in oral drug exposure following surgery and highlighted potentially important intrinsic factors that require further research in order to understand the post-surgical physiology. This would not have been made apparent had the results been published utilising only optimised systems parameters. It can therefore be argued that the aim of PBPK M&S within a systems pharmacology framework should not only be limited to the ability of predicting retrospective clinical data but it is of equal importance as a scientific framework for hypothesis generation.

An emerging body of evidence has been published supporting the impact of gastrointestinal hormones on physiological function, this can become crucial in fully unravelling the impact of bariatric surgery on oral first-pass effects as several hormones have been confirmed to affect intestinal physiological parameters whereas the quantitative data concerning the relationship between gastric hormone levels and systems parameters are at its best limited (Savage *et al.*, 1987; Sanger and Lee, 2008). The Medical Research Council (MRC) has identified bariatric surgery as a research tool for understanding the mechanisms of obesity and related diseases and the neuroscience of obesity. The developed PBPK models for bariatric surgery that are presented in this

thesis may provide a framework for linking physiological and hormonal data to oral drug delivery to potentially assist future research efforts (MRC, 2013).

Developed post bariatric surgery PBPK models provide a framework for theoretical exploration of physiological mechanisms associated with altered oral drug exposure pre to post surgery, which could be assigned to the interplay between dissolution, absorption and gut-wall metabolism, where dissolution and formulation properties emerged as the perhaps most important parameters in predicting the exposure following surgery.

At its full potential, post bariatric surgery models can be utilised for optimisation of pharmacotherapy, facilitating clinical decision making, and drug regulation. It may be postulated that this would be an area of particular relevance for the prediction of oral exposure of antidepressants as emerging clinical evidence suggest this drug class to display a reduced oral drug exposure following RYGB whereas they remain clinically relevant following surgery (Malone and Alger-Mayer, 2005; Darwich *et al.*, 2012a; Roerig *et al.*, 2012; Roerig *et al.*, 2013).

The utilisation of bariatric surgery PBPK models in clinical pharmacotherapy could partly be made possible due to user interface improvements in population-based PBPK software such as the Simcyp[®] Simulator, albeit usage may be restricted due to the required expertise to carry out M&S of novel compounds. The systems pharmacology approach does however provide complimentary advantages in addition to population pharmacokinetic approaches that have been used for clinical dose optimisation, such as the RightDose[™] software developed at the University of Southern California Laboratory of Applied Pharmacokinetics, by allowing mechanistic-based extrapolation along with estimates of population variability (Hope *et al.*, 2013).

In conclusion developed post bariatric surgery models provide a framework for studying mechanisms involved in the alteration of oral drug exposure and potentially provides a framework for pharmacotherapeutic drug optimisation. The relative success in modelling of oral drug exposure in post bariatric surgery patient populations further serves as a validation of the utilised template model, ADAM, incorporated into the

Simcyp[®] Simulator, through the successful prediction of oral drug exposure in a perturbed model system (Jamei *et al.*, 2009; Tsamandouras *et al.*, 2013).

7.2 Development of a nested enzyme-within-enterocyte model for predicting MBIs

A mechanistic model was developed to describe the hierarchical interdependency between enterocyte and enzyme turnover in the small intestine and its impact on the prediction of enzyme recovery following mechanism-based inhibition as compared to the conventional PBPK approach to modelling MBIs where enzyme and enterocyte turnover are lumped into a single rate of renewal as determined via indirect data in the form of clinical MBI studies.

The developed nested enzyme-within-enterocyte (NEWE) model is to the authors' knowledge the first model to differentiate between the first-order renewal of CYP enzyme activity and the zero-order turnover of the enterocytes in the small intestine following mechanism-based inhibition, thus avoiding the misspecification resulting from the lumping of these two physiological processes into a first-order rate.

Utilising the developed NEWE model, a lower level of inhibition of CYP3A following MBI was predicted during simulations as had been postulated. The predicted enzyme recovery using the NEWE model may potentially account for reported overpredictions in the level of mechanism-based inhibition as seen utilising static and dynamic modelling approaches coupled to IVIVE (Obach *et al.*, 2007; Fahmi *et al.*, 2009; Obach, 2013).

Uncertainties emerged regarding the parameter estimates of enzyme turnover as these were limited to *in vitro* data from cultured hepatocytes and human liver microsomes. It was further unclear what the consequences of enzyme inhibition would be on the substrate specific metabolic extraction in the gut wall where nonlinearity between enzyme activity and F_G may exist. This may be addressed through further model assessment and application, exploring the impact of NEWE model predictions subject to substrate specific metabolism.

Regardless, the model provides a more mechanistic description of enzyme recovery following mechanism-based enzyme inhibition in the small intestine where systems parameters are derived utilising a systems pharmacology approach rather than parameter estimation informed via indirect clinical data. The model can be utilised to predict the extent of gut wall metabolism and DDIs for orally administered drugs in special disease populations where enzyme or enterocyte turnover may be altered.

7.3 Principles and concepts of physiologically-based pharmacokinetic modelling and simulation

In this thesis, it was demonstrated that the systems pharmacology approach provides a potentially useful tool in the extrapolation and mechanistic exploration of the gastrointestinal component of F_{oral} in special subpopulations and theoretical modelling scenarios, such as the NEWE model development.

More mechanistic and highly specialised PBPK models have emerged in recent years to address scientific queries regarding special subpopulations and disease modelling. This has been made possible due to interdisciplinary efforts in the areas of systems biology, pharmacology and PBPK modelling, with the result of PBPK models with increasing levels of complexity *e.g.* type II diabetes, cardiac safety, hormonal responses, enterocyte maturation and more (Gadkar *et al.*, 2007; Shoda *et al.*, 2010; Machavaram *et al.*, 2013; Polak, 2013; Chen *et al.*, 2014). Implemented modelling approaches throughout this thesis clearly conform to this trend and motivates the discussion of some of the underlying principles that make up PBPK M&S and systems pharmacology, and where PBPK will be heading in future.

‘Top-down’ versus ‘bottom-up’ and meeting in the middle

The utilisation of PBPK M&S under the principles of systems pharmacology is often referred to as a ‘bottom-up’ approach, where model specification and parameterisation is based on physiological data, IVIVE and IVIVC. The ‘bottom-up’ approach may, philosophically and in principle, be considered the flip-side of the empirical compartmental modelling approach, referred to as the ‘top-down’ approach.

These two approaches do however serve distinct purposes in PK M&S, where ‘bottom-up’ has the inherent advantages of allowing mechanistic interpretation and facilitating extrapolation, including: IVIVE, interspecies and between population extrapolation, such as the case of bariatric surgery and DDIs as exemplified in this thesis where clinical data may be sparse. The ‘bottom-up’ approach is however extremely ‘data hungry’, requiring data from interdisciplinary sciences in order to populate and give confidence to systems parameters, there has however been an easement over the last decades due to the development and refinement of IVIVE, IVIVC and *in silico* methods for parameter predictions based on PhysChem data.

Utilising a ‘top-down’ approach an empirical model can be derived solely based on clinical data, producing estimates of population parameters and their variability. The success of the approach is however highly dependent on the clinical data and does not enable extrapolation to other study populations. The ‘top-down’ approach is highly advantageous in clinical research where it may be utilised for optimal design of late-stage clinical trials and covariate analysis.

The perhaps more pragmatic and viable approach is to utilise a data driven modelling approach where the angle from which the problem is tackled may be chosen based on available data and the aim of the modelling exercise. Depending on available data, model parameters may be derived using a physiologically-based approach or parameter estimation methods inferred from clinical data, this approach is often referred to as the ‘middle-out’ approach. One of the main challenges of utilising such a ‘middle-out’ approach is the issue of structural identifiability, where a complex PBPK model structure may not enable the unique identification of a single ‘true’ parameter value, or global optima. Further, complex PBPK models may not be sensitive to specific parameter estimates due to the intrinsic sensitivity of the structural model or design of associated clinical data. An important consideration when estimating parameters in a PBPK model is the correlation between parameters, where for example a substrate’s affinity to a particular enzyme should not differ in different tissues. These issues may be overcome to a varying extent by altering the structural model or through reparameterisation, designing experiments to inform the model or the usage of prior knowledge to inform model parameters thus restricting parameters within plausible ranges (Yates, 2006; Tsamandouras *et al.*, 2013).

To examining the PBPK M&S cases in this thesis it was prerequisite to utilise a ‘bottom-up’ approach as the modelling tasks were concerned with the extrapolation of drug disposition between populations and exploratory M&S albeit some elements of ‘middle-out’ approach were implemented due to the utilisation of parameter estimation concerning transporter activity. Due to the complexity of the model concerns regarding the structural identifiability of estimated parameters may be justified as is the general concern when estimating parameters of a full PBPK model. Estimated parameters concerning transporter activity were not possible to scale using IVIVE due to the lack of absolute transporter abundance data in man. Estimations could however be considered to lie within plausible ranges.

External versus internal tools

The research carried out in this thesis further showcase the utilisation and respective benefits of external and internal tools in PBPK M&S. External tools can in short be described as externally developed M&S platforms consisting of a set of predefined models that may be utilised and perturbed to varying extent, *e.g.* Simcyp[®] Simulator and GastroPlus[™]. Internal tools provide a more general modelling environment for custom model development and usually involve the utilisation of a high-level programming language, such as Matlab and R, but may also provide model development through a graphical user interface, such as the case for SAAM 2. This is not to be confused with commercial versus open-source software platforms as toolsets may exist in both forms (Vicini *et al.*, 2013).

External and internal PBPK M&S tools have their distinct advantages and disadvantages. External tools provide several advantages, including the provision of a general framework for PBPK M&S consisting of widely recognised modelling approaches and procedures. In general, external models are also populated with parameters from rich datasets, thus providing more reliable estimates of systems parameters and their variability. This enables modellers, reviewers and regulatory bodies with ease of interpretation of model development and outcomes, and reproducing results. As external tools generally provide user-friendly interfaces the toolset are more readily available for non-modellers, this is of particular importance in PBPK where the

discipline relies on the generation of parameter data from interdisciplinary sciences (Vicini *et al.*, 2013).

One of the main disadvantages with the utilising of external tools is that these in general provide highly specific frameworks for modelling which may be considered a ‘black box’ if the user is not adequately trained in utilising provided models and tools (Vicini *et al.*, 2013).

The use of an external toolset was of particular benefit in the development of post bariatric surgery PBPK models as these were all developed through the perturbation of a highly complex absorption model, it was therefore essential for the models to be populated by well-characterised systems parameters in order to estimate population variability. The user-friendly interface may further be an advantage if the models are to be implemented by non-modellers in a clinical setting. The main limitation was the lack of flexibility that the external tool provided where certain aspects of alterations in fluid dynamics (altered luminal secretion and reabsorption) could not be tested.

The most apparent advantage of utilising an internal PBPK M&S toolset is the inherent flexibility in model development and customisation. This may be particularly suitable for testing novel modelling concepts and ideas, such as the case of the NEWE model described above, or performing modelling tasks outside the general framework of PBPK. Providing that a published model is adequately described reproduction may be considered a non-issue, this does however require adequate expertise in utilising the programming language of an internal toolset and may therefore make interpretation and reviewing more difficult. An additional disadvantage of internal tools is the lack of the volume of data and analysis that has gone into populating the parameters of an external tool. As external M&S tools are developing into more flexible working environments the distinction between the two toolsets is becoming less apparent where both toolsets may for example facilitate a ‘middle-out’ model development approach, as exemplified in this thesis where parameters for the tissue disposition of atorvastatin acid could be estimated in order to infer missing data (Vicini *et al.*, 2013).

General framework and the regulatory view on PBPK M&S

In recent years there has been a significant increase in the usage of PBPK models by regulatory bodies and pharmaceutical industry to support regulatory submissions and prescribing information for dose optimisation, DDI predictions and extrapolation to special populations. PBPK M&S has now for the first time been utilised in drug labelling to singlehandedly inform outcomes following DDIs. Due to cost and practical issues with recruitment not all physiological conditions where several physiological factors vary from the norm can be investigated through clinical studies to inform drug labelling. This extends to post bariatric surgery patient populations where patient numbers are increasing rapidly whereas patient recruitment can be cumbersome. FDA highlighted some of the issues that need to be overcome in order for PBPK M&S to reach its full potential, this includes: a better understanding of off target effects and drug disposition, integration of 'bottom-up' and 'top-down' modelling approaches, education and training, sharing of data between academia industry and government, better procedures for model evaluation, and the development and utilisation of general frameworks and best practices in PBPK M&S (Huang *et al.*, 2013; Pharmacocyclics, 2013).

In 2011 FDA published a general scheme for PBPK model development based on lessons learned from earlier reviewed submissions of new drug applications and investigational new drugs. The general framework for PBPK subsequent fashion included: identification and quantification of clearance pathways, incorporation of drug dependent parameters into a PBPK model, comparison of concentration-time profiles to clinical data and finally the utilisation of refined PBPK model to predict drug disposition (Zhao *et al.*, 2011).

FDA also highlighted the increasing availability of PBPK models for special population due progress made in systems biology and pharmacology. Model development of special population models requires the identification of population specific extrinsic and intrinsic factors in order identify and characterise systems parameters, this will be followed by a general model development framework, incorporating systems and drug-specific parameters into a PBPK model followed by stages of predictions, learning and confirmation (Zhao *et al.*, 2011).

A similar framework was drawn up by the WHO in an attempt to harmonise the development of PBPK models for risk assessment. The postulated workflow put particular emphasis on problem evaluation and the need for purpose specific validation and evaluation (WHO, 2011).

The development of post bariatric surgery PBPK models took on a very similar approach, where the identification of the modelling aim was followed by problem evaluation in the form of a literature review and statistical meta-analysis, the identification of relevant intrinsic factors and their characterisation, model development, assessment and validation. In the case of bariatric surgery it is of particular interest to note its potential usage in identifying ‘known unknown’ intrinsic factors. As more data emerges further model refinements will be made possible. The systems pharmacology approach should be subject to constant review and revision of both models and parameter values in order to remain current as a tool for exploration and extrapolation.

Further, it should be emphasised that the model development for special populations should not be considered a problem constrained to population specific systems parameters. It is also critical to identify and characterise relevant drug and formulation-specific parameters that may interact with the altered systems parameters in order to answer the purpose specific questions, e.g. In order to draw well-founded conclusions regarding changes in F_G following bariatric surgery necessary metabolic assay *in vitro* data is required.

7.4 Final conclusions

A systems pharmacology approach was used in order to explore the GI component making up oral drug delivery. The impact of f_a and F_G on F_{oral} was explored through the successful implementation of PBPK models for a morbidly obese patient population subject to bariatric surgery and a mechanistic model describing the recovery of enzyme activity following mechanism-based inhibition using a nested enzyme-within-enterocyte turnover model of the small intestine. Developed models showcase the advantage of PBPK M&S in the extrapolation of oral drug exposure to special population and potential of the approach in understanding underlying the underlying mechanism governing oral drug delivery.

7.5 Future work

During the development and application of post bariatric surgery PBPK models a number of potential areas of further research presented themselves, these included: The quantitative modelling of gastric hormones and their effect on gastrointestinal systems parameters relevant to drug disposition and model application on the predicted oral exposure of antidepressants. Further, it would be of great interest to explore the potential of implementing a PBPK M&S framework in a clinical setting to optimise clinical pharmacotherapy.

Although assessment of the NEWE model suggested its potential for improving the prediction of enzyme recovery in the gut wall following mechanism-based inhibition further work is required to determine the predicted impact on substrate specific extraction in the gut wall and its ability to reproduce clinical outcomes. This should be done through model further model assessment exploring substrate specific F_G and validation against clinical MBI data.

In addition, the exploratory assessment of developed PBPK models identified areas of where our current understanding is lacking that may therefore require further research. Data is currently very limited with regards to the mechanistic and quantitative relation between gastric hormones, gastrointestinal physiology and how altered hormonal levels will affect the post bariatric surgery physiology short and long-term. Areas of interest for further research would also include: intestinal transit and fluid dynamics following bariatric surgery, the long-term adaptation of the gastrointestinal tract following bariatric surgery, and the characterisation of enzyme turnover in the small intestine independent from enterocyte turnover.

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Chapter 8: Appendices

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8.1 Trends in oral drug bioavailability following bariatric surgery: examining the variable extent of impact on exposure of different drug classes

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Trends in oral drug bioavailability following bariatric surgery: examining the variable extent of impact on exposure of different drug classes

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WHAT IS ALREADY KNOWN ABOUT THIS SUBJECT

- Changes to oral drug bioavailability have been observed post bariatric surgery. However, the magnitude and the direction of changes have not been assessed systematically to provide insights into the parameters governing the observed trends. Understanding these can help with dose adjustments.

WHAT THIS STUDY ADDS

- Analysis of drug characteristics based on a biopharmaceutical classification system is not adequate to explain observed trends in altered oral drug bioavailability following bariatric surgery, although the findings suggest solubility to play an important role.

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AIMS

To identify the most commonly prescribed drugs in a bariatric surgery population and to assess existing evidence regarding trends in oral drug bioavailability post bariatric surgery.

METHODS

A retrospective audit was undertaken to document commonly prescribed drugs amongst patients undergoing bariatric surgery in an NHS hospital in the UK and to assess practice for drug administration following bariatric surgery. The available literature was examined for trends relating to drug permeability and solubility with regards to the Biopharmaceutics Classification System (BCS) and main route of elimination.

RESULTS

No significant difference in the 'post/pre surgery oral drug exposure ratio' (ppR) was apparent between BCS class I to IV drugs, with regards to dose number (Do) or main route of elimination. Drugs classified as 'solubility limited' displayed an overall reduction as compared with 'freely soluble' compounds, as well as an unaltered and increased ppR.

CONCLUSION

Clinical studies establishing guidelines for commonly prescribed drugs, and the monitoring of drugs exhibiting a narrow therapeutic window or without a readily assessed clinical endpoint, are warranted. Using mechanistically based pharmacokinetic modelling for simulating the multivariate nature of changes in drug exposure may serve as a useful tool in the further understanding of postoperative trends in oral drug exposure and in developing practical clinical guidance.

Introduction

Obesity is generally defined by the body mass index (BMI = body weight (kg)/height (m)²). The classification is somewhat arbitrary such that 'overweight' means a BMI ≥ 25 but <30 kg m⁻², 'obesity' refers to BMI ≥ 30 but <40 kg m⁻² and 'morbid obesity' is a BMI ≥ 40 kg m⁻² (this may also refer to being obese and suffering from related co-morbid conditions) [1, 2]. Over the last decade the prevalence of obesity has increased dramatically in the USA and Europe. In the USA 32.2% of the male and 35.5% of the female population over the age of 20 years were characterized as obese in 2007–2008 [3]. The United Kingdom has the highest reported obesity rate in Europe [4]. In England, 24.1% of the male and 24.9% of the female population over the age of 16 years were classified as obese in 2008 [5]. Bariatric surgery has proven to be successful in treating morbid obesity. In the USA and Canada approximately 200 000 bariatric surgeries were performed in 2008 [6]. In England 4221 surgeries were performed in 2008/09, an increase of over 100% since 2006/07 [1, 7]. Several bariatric surgical methods currently coexist in healthcare. These include the adjustable gastric band (AGBD), sleeve gastrectomy (SG), biliopancreatic diversion (BPD), biliopancreatic diversion with duodenal switch (BPD-DS) and Roux-en-Y gastric bypass (RYGB) [8]. Other procedures, such as jejunoileal bypass (JIB), have been gradually phased out due to a higher likelihood of adverse events [9–11].

Bariatric surgical procedures have been well described in the literature [11, 12], where they are generally characterized as being restrictive, in terms of physiologically reducing dietary intake, malabsorptive, through reducing the ability of the gastrointestinal (GI) tract to absorb nutrients or a combination of both.

Restrictive procedures such as AGBD and SG result in a reduced gastric capacity to 15–20 ml and 60–80 ml respectively [12, 13]. The JIB, considered a malabsorptive procedure, results in a 90–95% bypass of the small intestine, retaining the duodenum, proximal jejunum and terminal ileum [9–11]. The BPD-DS, primarily a malabsorptive procedure, results in a reduced gastric volume (100–175 ml) and bypass of larger parts of the small intestine, forming a biliopancreatic canal transporting the bile juices to the distal ileum [14, 15]. The RYGB, combining restriction and malabsorption, results in the restriction of the stomach to 15–30 ml and bypass of the proximal small intestine [15–17].

Bariatric surgery imposes a number of physiological alterations known to affect the bioavailability of orally administered drugs (F_{oral}), dependent on the fraction of drug that is absorbed in the intestinal gut wall (f_a), the fraction that escapes gut wall metabolism (f_g), and the fraction that escapes hepatic metabolism (f_H) (Equation 1).

$$F_{\text{oral}} = f_a \cdot f_g \cdot f_H \quad (1)$$

f_a and f_g are highly influenced by drug specific properties, such as permeability and solubility, and the GI physiology such as gastric emptying time, GI pH profiles, small intestinal transit time, GI drug metabolizing enzymes and GI efflux transporters [18, 19]. Gastric emptying time can serve as the rate limiting step for highly permeable and highly soluble drugs as the absorption from the stomach is low [20]. The gastrointestinal pH may affect drug dissolution of permeability-limited drugs displaying a pKa within the range of the GI pH fluctuations. Small intestinal transit time can influence the drug absorption of poorly soluble or extended release drug formulations [18].

Metabolism in the gut acts to regulate oral bioavailability of drugs and other xenobiotics, and is an important determinant in the metabolism of substrate drugs [21]. CYP3A4 is the most abundant drug metabolizing enzyme in the GI tract, preceding CYP2C9/19 amongst others in order of appearance [22–25]. CYP3A4 and CYP3A5 are both present along the GI tract, where CYP3A4 expression rises towards the jejunum to decrease towards the ileum [21, 26]. GI transporters may influence the absorption of orally administered drugs and potentially also the extent of metabolism in the gut through active substrate efflux [27]. Numerous transporters are present in the gut, where P-glycoprotein (P-gp) is perhaps the most extensively studied of the GI transporters. The relative expression pattern of P-gp in the small intestine increases from the proximal to the distal parts of the small intestine [28].

The Biopharmaceutics Classification System (BCS) classifies drugs in accordance with their solubility and permeability. Solubility takes on the form of a dose number (Do), given by dividing highest dose strength in mg (M_o) by a volume of 250 ml (V_o) divided by the aqueous solubility of the drug (mg ml⁻¹) over a pH range of 1.0–7.5 at 37°C (C_s) [29]. Defining $Do \leq 1$ as highly soluble and an $f_a \geq 90\%$ as a highly permeable drug, drugs are classified as Class I (high solubility-high permeability), class II (poor solubility-high permeability), class III (high solubility-poor permeability) and class IV (poor solubility-poor permeability) [30].

The aims of this study were to identify the most commonly prescribed drugs in a bariatric surgery population and to assess existing evidence with respect to altered oral drug bioavailability post bariatric surgery. This would be carried out through methodologically reviewing the current literature, evaluating drug specific pharmacokinetic characteristics relating to solubility, permeability and main route of elimination.

Methods

Evaluation of drug utilization following gastric bypass

A retrospective audit of drug utilization by bariatric surgery patients was performed at Salford Royal NHS

Foundation Trust, Salford, UK. Data collection was performed using the hospitals electronic patient record (EPR) system, iSOFT clinical manager 1.4, which incorporates the medication prescription and administration records. A search of the EPR system was carried out for all patients under the care of a consultant bariatric surgeon. The search consisted of patients who had undergone surgery in the previous 5 months, from the 21 March 2011. The medical history of patients was initially searched to identify those having undergone laparoscopic RYGB. Patients who had a colostomy, gastric banding and reversal of gastric banding were excluded.

Data extraction was performed utilising an anonymous data collection form, maintaining patient confidentiality. Information extracted consisted of type of bariatric surgical procedure, pre surgery prescribed drug therapy and associated co-morbidities, post surgery medication including formulation changes and documented reasons behind alterations. Pre surgery medications were compared with the patients' medical charts on discharge, generally 2–3 days post surgery. Statistical analysis of trends in prescribed drugs observed during the retrospective audit was conducted using McNemar's non-parametric test ($P \leq 0.05$) in R v 2.12 (the R Foundation for Statistical Computing).

Review and analysis of oral drug bioavailability following gastric bypass

Embase (1980–2010) and PubMed (1977–2010) were searched using the following combinations of keywords: 'oral administration or bioavailability', 'absorption', 'bioavailability', 'gastric bypass', 'jejunoileal bypass', 'bariatric surgery'. In addition, references of related articles were systematically investigated for relevant publications.

Initial screening of titles and abstracts was carried out to identify those compliant with pre specified criteria of reporting observational trends in bioavailability/oral drug exposure of pharmaceutical agents following bariatric surgery or the identification of adverse events related to oral drug exposure following surgery. Studies excluded consisted of gastric surgical procedures not related to obesity, reports on nutrients or supplementation post bariatric surgery and publications written in a language other than English. Screening was carried out to determine inclusion or exclusion criteria. Information extracted included study characteristics (surgical procedure, study design, number of participants, year of publication, country of origin and time since procedure) and study population characteristics (gender, average age, average body mass index (BMI) and co-morbidities). The principle measurement of bioavailability in the analysis was area under the curve (AUC), bioavailability and steady-state plasma or serum concentration.

Observed trends in oral drug exposure were assumed to follow a log normal distribution. Quantitative analysis was carried out through estimating the mean effect size of

response ratios and their variance following a random-effect model. Statistical analysis was carried out with a two-tailed *t*-test of the standard normal cumulative distribution [31]. Statistical analysis between subgroups were carried out utilizing Welch's *t*-test ($P \leq 0.05$) of log-transformed weighted means and SDs with *post hoc* Dunn-Šidák correction ($P \leq 0.05$) using Microsoft® Excel 2003 and Matlab 2010 (the Mathworks Inc).

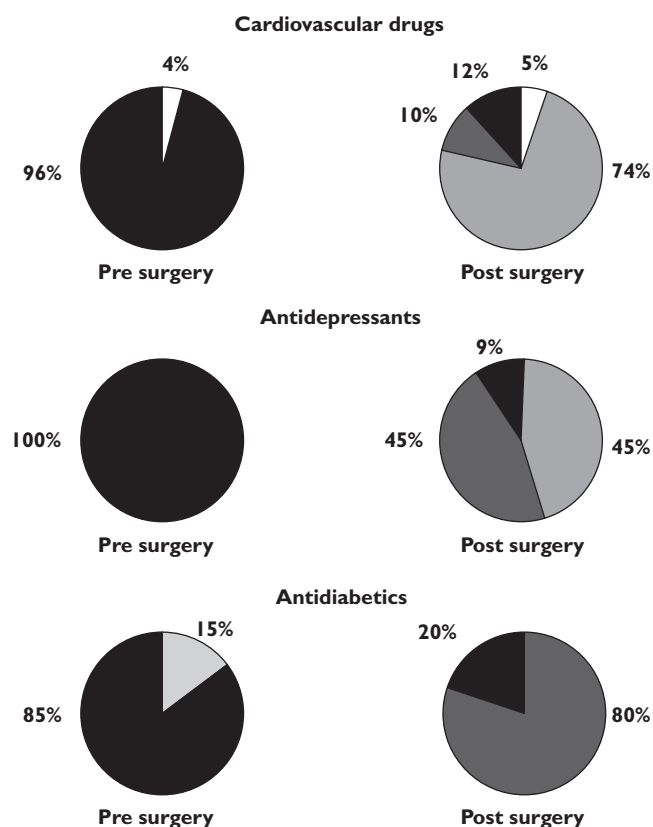
Results

Evaluation of clinical drug utilization following gastric bypass

The search of iSOFT identified 63 patients under the care of the bariatric surgeon and 38 patients (26 female) with a mean age of 45 (range 23–64) years were eligible for data extraction after fulfilling the pre-specified criteria. The surgical procedures performed included laparoscopic RYGB ($n = 34$), laparoscopic RYGB with abdominal wall hernia repair ($n = 3$) and conversion of AGBD to RYGB ($n = 1$). Commonly treated comorbidities amongst the study population included hypertension ($n = 12$), type 2 diabetes ($n = 15$), depression/anxiety ($n = 11$), hypothyroidism ($n = 5$), osteoarthritis ($n = 11$), hypercholesterolaemia ($n = 10$) and asthma ($n = 9$).

The most commonly prescribed drugs prior to surgery included statins ($n = 13$), ACE inhibitors ($n = 10$), proton pump inhibitors (PPIs)/histamine H₂-receptor antagonists ($n = 10$) and metformin ($n = 10$). Comparing pre to post surgery, a significant increase in the prescription of paracetamol, opioids, PPIs/histamine H₂-receptor antagonists, heparin and antimicrobials was observed ($P < 0.05$) as well as an overall reduction in the number of patients treated for type 2 diabetes ($P < 0.05$). The most common drugs prescribed following surgery included heparin ($n = 38$), PPIs/histamine H₂-receptor antagonists ($n = 38$) and paracetamol ($n = 34$). The number of patients prescribed cardiovascular agents remained constant postoperatively, whereas prescriptions of statins displayed a non-significant reduction of 31% ($P > 0.05$). The postoperative formulation of choice for diuretics was liquid ($n = 4$), whereas the remaining cardiovascular agents were tablets that were being crushed postoperatively ($n = 28$) (Figure 1).

All patients receiving antidepressants remained on the same antidepressant post surgery, with all but one receiving a different formulation. Of the 11 patients prescribed antidepressants, 50% were switched on to liquid formulations, whereas the remaining 50% were advised to crush their tablets post surgery (Figure 1). All patients with a prior diagnosis of diabetes underwent a diabetic review during their stay in hospital. The review resulted in a significant reduction in post-surgical prescriptions of anti-diabetic medications by 67% ($P < 0.05$). Patients who no longer required diabetic medication were alternatively switched to manual monitoring of blood glucose concen-

**Figure 1**

Pharmacotherapeutic alterations in formulation properties (Solid = solid tablets, Liquid = liquid formulation, S/C = subcutaneous, Crushed = patients instructed to crush tablets, Inhaled = inhalation formulation) post bariatric surgery of prescribed cardiovascular drugs, antidepressants and antidiabetics as compared with prior to surgery observed in 38 evaluated patients. Solid (■); Liquid (■); Crushed (■); S/C (■); Inhaled (□)

trations. Metformin was the only agent continued postoperatively and in 60% of cases continued at a reduced dose of up to a third of the pre-surgical dose level. All but one patient were converted to liquid preparations (Figure 1). Standard postoperative treatment consisted of 1–2 weeks low molecular weight heparin injection, PPIs (lansoprazole FasTab) and liquid formulation pain-killers (codeine and paracetamol) being prescribed for all patients. This patient group also displayed a significant increase in the prescription of PPIs/histamine H₂ receptor antagonists, opioids, paracetamol and heparin ($P < 0.05$). One patient with a history of deep vein thrombosis remained on tinzaparin for 4 weeks.

Lansoprazole was given at a dose of 30 mg twice daily as a orodispersible formulation. The prophylactic therapy was to continue for at least 6 months postoperatively, before reducing the dose to once daily for a further 18 months. Approximately 2 weeks after surgery the sublingual formulation was switched to the solid tablet or capsule formulation.

Antimicrobials were given to seven patients postoperatively for the eradication of *Helicobacter pylori* ($n = 5$) that was detected from an intra-operative gastric mucosal biopsy, development of hospital-acquired pneumonia ($n = 1$) and anastomotic leakage ($n = 1$). All patients were given liquid preparations.

In total 17 patients were taking analgesics on a regular basis prior to surgery, increasing to 38 patients postoperatively. Analgesic products included paracetamol ($n = 2$, $P < 0.05$), aspirin ($n = 5$), opioids ($n = 9$, $P < 0.05$) and non-steroidal anti-inflammatory drugs (NSAIDs) ($n = 3$). Patients taking NSAIDs prior to surgery ($n = 3$) were advised to stop taking these postoperatively due to an increased risk of developing gastro-jejunal anastomotic ulceration.

As stated in the patients 'plan' for postoperative care, a review of the nutritional progress usually occurred approximately 2 weeks post surgery. Patients were therefore advised to cease taking any non-essential vitamins and minerals immediately after surgery until the nutritional review has been completed. On discharge patients were informed that they would require taking lifelong dietary supplementation.

Oral drug bioavailability following bariatric surgery

The initial search of Embase and PubMed identified 311 potentially relevant publications based on search terms. After screening of abstracts, 66 articles were identified of which 22 matched the pre-specified criteria following full text screening. Overall, the literature search included 41 articles (20 controlled trials, 18 case reports and three case series) published between 1974 and 2011 that were suitable for further evaluation and data extraction.

Articles relating to JIB mainly appeared between 1974 and 1985. An increase of published data on RYGB was identified between 2000 and 2011, following the trend of RYGB being the most widely used bariatric surgical procedure at the present time [1].

Surgical techniques identified included RYGB ($n = 14$), JIB ($n = 19$), reversal of jejunoileal bypass (JIB R) ($n = 4$), BPD-DS ($n = 2$) BPD ($n = 3$), GBP ($n = 1$) and AGB ($n = 1$) (Table 1). The 41 identified publications originated from the USA (58%), followed by the UK (10%), Italy (5%), Norway (5%) and Canada (5%).

A total of 230 participants were studied in the identified publications. The time point for post surgical examination of oral drug exposure ranged from 0.1 to 88.9 months [32, 33]. In total 38 drugs were identified. These were categorically divided based on therapeutic indication. The studied drugs consisted of antimicrobials ($n = 12$ drugs), cardiovascular drugs ($n = 2$), immunosuppressants ($n = 4$), antiepileptics ($n = 3$), analgesics ($n = 2$), oral contraceptives ($n = 4$), anti-ulcer drugs ($n = 1$), statins ($n = 1$), thyroid hormones ($n = 1$), antidepressants ($n = 2$), anti-cancer drugs ($n = 2$), anti-diabetics ($n = 1$) and HIV medication ($n = 1$). Postoperative trends in drug bioavailability based on

Table 1

Controlled trials examining the trend in oral drug exposure following bariatric surgery.

	Drug	Surgery	Pre to post surgery oral drug exposure ratio (X, 95% CI)	Patients (n)	References
▲	Phenoxymethyl penicillin 1000 mg	JIB	10.43 (0.10, 1058)*	3	[34]
	Atorvastatin acid 20–80 mg	BPD-DS	1.85 (0.81, 4.27)†	10	[36]
—	Ranitidine 300 mg	BPD	1.43 (1.12, 1.81)*	11	[40]
	Metformin 1000 mg	RYGB	1.20 (0.91, 1.58)†	16	[55]
	Propylthiouracil 400 mg	JIB	1.09 (0.84, 1.42)†	6	[90]
	Phenazone 15 mg kg ⁻¹	JIB	1.06 (0.81, 1.38)‡	17	[91]
	Atorvastatin acid 20–80 mg	RYGB	1.00 (0.29, 3.46)†	12	[37]
	Paracetamol 1500 mg	JIB	1.00 (0.647, 1.54)*	3	[34]
	Digoxin 0.5 mg daily (First day: 1 mg)	JIB	0.89 (0.70, 1.14)†	7	[39]
	Erythromycin 250 mg	GBP	0.61 (0.38, 0.99)†	7	[92]
▼	Sulfisoxazole 1000 mg	JIB	0.84 (0.74, 0.94)*	3	[93]
	Norethisterone 3 mg	JIB	0.80 (0.39, 1.63)‡	6	[94]
	Digoxin 0.5 mg	JIB	0.76 (0.59, 0.97)†	9	[38]
	MMF 2-1000 mg	RYGB	0.66 (0.21, 2.06)*	2	[33, 95]
	Levonorgestrel 0.25 mg	JIB	0.55 (0.34, 0.90)‡	6	[94]
	Sirolimus 8 mg	RYGB	0.54 (0.25, 1.17)*	4	[33, 96, 97]
	Hydrochlorothiazide 75 mg	JIB	0.46 (0.33, 0.65)*	4	[98, 99]
	Sertraline 100 mg	RYGB	0.40 (0.19, 0.84)†	5	[100]
	Ampicillin (pivampicillin 750 mg)	JIB	0.37 (0.16, 0.89)†	5	[90]
	Phenytoin 200 mg	JIB	0.32 (0.17, 0.58)†	7	[101]

▲ = Indicating a significant increase in oral drug exposure (AUC, F_{oral} or steady-state concentration) following surgery. — = No statistical significant change in oral drug exposure.

▼ = Significant reduction in oral drug exposure. X = mean ratio change based on geometric mean, GBP, Gastric bypass (gastroplasty and Roux-en-Y gastric bypass); JIB, Jejunoileal bypass; BPD, Biliopancreatic diversion; BPDDS, Biliopancreatic dDivision with a duodenal switch; RYGB, Roux-en-Y gastric bypass; MMF, mycophenolate mofetil. *t-test performed at 5% significance level. †Statistical outcome as reported in publication. ‡Welch's t-test at a 5% significance level.

geometric mean drug exposure ranged from a 10.43 fold increase with a 95% confidence interval (CI) ranging from 0.10 to 1058 ($n = 32$) [34] to a 5.88 fold reduction ($n = 1$) [35] (Table 1) [36–41]. The overall post/pre surgical oral drug exposure ratio (ppR) obtained from meta-analysis significantly diverged from pre surgery with a mean ppR of 0.80 with a 95% CI of 0.67, 0.94 (z value = -2.65 , $P < 0.01$), when analyzing quantitative data providing mean and variance of exposure pre and post bariatric surgery.

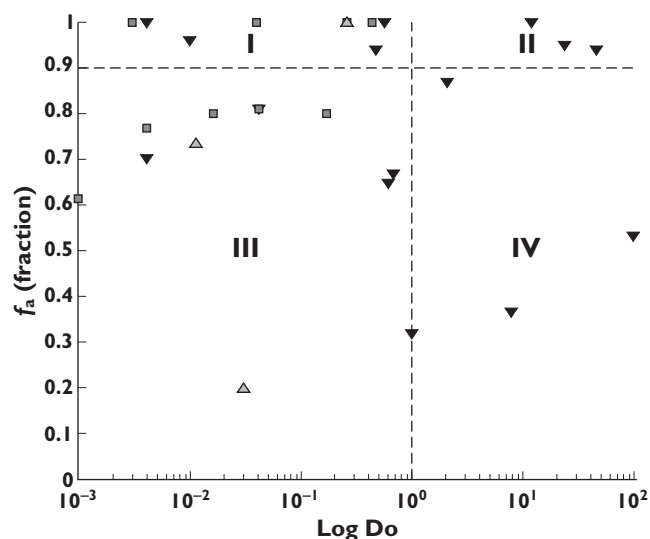
Analysis in accordance to the Biopharmaceutics Classification System Classifying drugs into BCS classification, class I (high solubility, high permeability), class II (low solubility, high permeability), class III (high solubility, low permeability) and class IV (low solubility, low permeability), identified eight drugs as BCS class I ($n = 66$ patients), three drugs as BCS class II ($n = 7$), eleven drugs as BCS class III ($n = 53$) and three drugs as BCS class IV ($n = 8$). A total of eight drugs were found to be inconclusive ($n = 40$). Information was lacking in the literature with regards to the BCS classification of pivampicillin, para-aminosalicylic acid and lopinavir/ritonavir.

Of the eight drugs identified as BCS class I, four drugs displayed a reduction in exposure following surgery, four drugs remained unaltered and one drug displayed an increase in drug exposure. Out of eleven mapped BCS class III drugs, five displayed a reduction in drug exposure

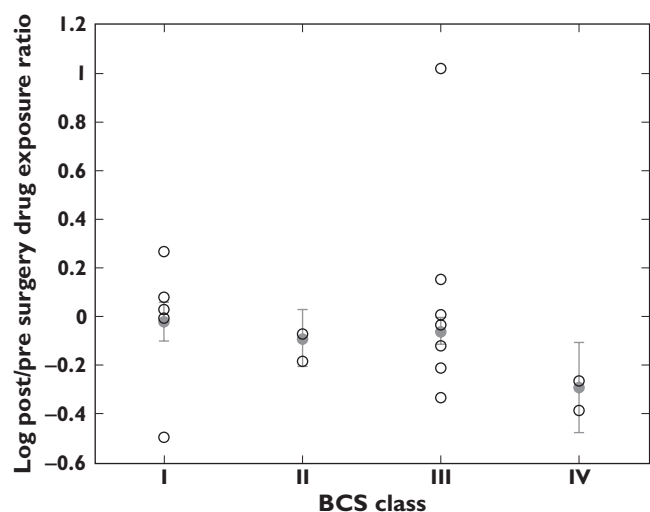
following surgery. An additional five drugs displayed unaltered drug exposure, whereas one drug displayed an increase. All BCS class II and IV drugs (total of six) displayed a reduction in drug exposure following surgery (Figure 2).

Analyzing BCS classified drugs where studies provided quantifiable measurements of drug exposure (*i.e.* AUC, F_{oral} and plasma or serum concentrations), combining weighted means and variance of pre/post drug exposure ratio, BCS class I ($n = 5$ drugs, $n = 108$ population) displayed a weighted mean ppR of 0.94 (95% CI 0.66, 1.34). BCS class II ($n = 2$ drugs, $n = 5$ population) displayed a weighted mean ppR of 0.80 (95% CI 0.48, 1.36), BCS class III ($n = 8$ drugs, $n = 111$ population) showed a weighted mean ppR of 0.86 (95% CI 0.68, 1.10), whereas BCS class IV ($n = 2$ drugs, $n = 17$ population) displayed a weighted mean ppR of 0.51 (95% CI 0.22, 1.17). Statistical analysis did not reveal any significant differences from pre surgical ratio of 1 between BCS subgroups ($P > 0.05$) (Figure 3).

Drugs where studies provided quantifiable measurements of drug exposure were further statistically analyzed with regards to $Do \leq 1$, BCS class I and III ($n = 16$ drugs, $n = 262$ population) vs. BCS class II and IV ($n = 4$ drugs, $n = 48$ patients). $Do \leq 1$ drugs displayed a weighted mean ppR of 0.83 (0.69–1.00), whereas $Do > 1$ drugs displayed a ratio of 0.70 (95% CI 0.45, 1.10). Statistical analysis revealed no statistical significance from a pre surgical ratio of 1 or between subgroups ($P > 0.05$) (Figure 4).

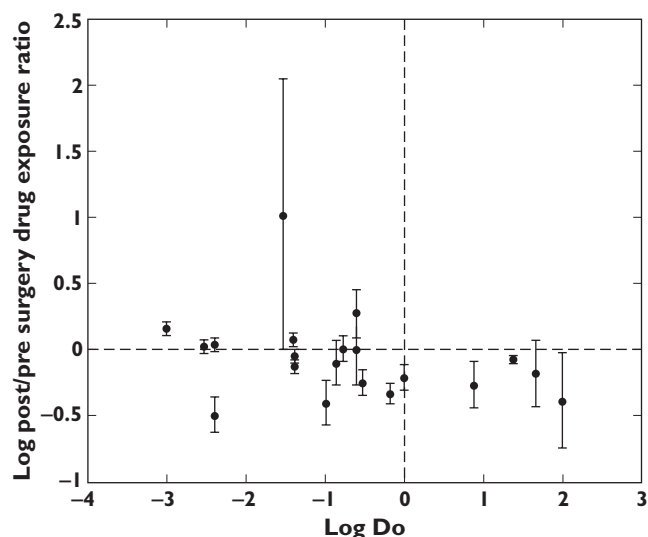
**Figure 2**

Categorical trends (reduced, unaltered and increased) in oral drug exposure in relation to f_a (fraction of orally administered dose absorbed) and Do (dose number) in accordance with the BCS dividing drugs into BCS class I–IV [52,60–89]. Reduced exposure (▼); Unaltered (□); Increased (△).

**Figure 3**

Log mean post/pre surgery drug exposure ratio of BCS I–IV classified drugs. ○ log mean drug ratio, ● combined log mean ratio and standard deviation of subgroup

Analysis in accordance to main route of elimination
Examining drugs in accordance with the main route of elimination produced a weighted mean ppR in oral drug exposure of 0.83 (95% CI 0.59, 1.17) for CYP3A4/5 substrates ($n = 7$ drugs, $n = 99$ patients), 0.32 (95% CI 0.14, 0.72) for CYP2C substrates ($n = 1$ drug, $n = 16$ population), 0.90 (95% CI 0.68, 1.18) for mainly renally-cleared drugs ($n = 5$ drugs, $n = 103$ population) and 0.76 (95% CI 0.57, 1.01) for the remaining drugs ($n = 8$ drugs, $n = 92$ population). Sta-

**Figure 4**

Mean post/pre surgery drug exposure ratio and standard deviation in relation to quantitative Do (dose number)

tistical analysis revealed no difference in ppR between the subgroups ($P > 0.05$), whereas the CYP2C subgroup significantly differed from the pre-surgical ratio of 1, displaying a z-value of -2.72 and $P < 0.001$.

Discussion

Evaluation of drug utilization following gastric bypass

The observed practice of altering formulation properties to liquid preparations is considered necessary in health-care due to the postoperative condition of the patient rather than as a proactive measure against altered pharmacokinetics due to changes in GI physiology. Patients are advised to remain on liquid formulations for approximately 2–3 weeks, varying nationally to 3 months to life-long, post bariatric surgery to prevent any unnecessary strain on the gastric and jejunal transection lines and the gastrojejunal anastomosis and therefore to allow time for healing. As an unintentional consequence changing to liquid preparations may result in an increase in oral bioavailability for solubility limited drugs.

Pharmacotherapeutic treatment of type 2 diabetes was ceased in 67% of patients following surgery. The prescription of metformin remained unaltered following surgery, albeit being observed to be significantly reduced 12 months postoperatively, by Malone & Alger-Mayer, following 114 patients up to 24 months post surgery [42].

Antidepressants, TCAs and SSRIs were continued immediately postoperatively in all cases. This was consistent with

the report by Malone & Alger-Mayer, indicating prescriptions of TCAs and SSRIs remained statistically unaltered 12 months post surgery. Vitamin and mineral deficiencies are likely to occur indefinitely in the bariatric patient, resulting in the need for lifelong supplementation [43]. Deficiencies are most likely to occur with fat soluble vitamins (A, D, E and K), calcium and iron. Calcium and iron absorption is highly influenced by the reduction of hydrochloric acid production within the stomach after bariatric surgery [43].

Medication reviews have been performed observing modifications to patient dosing and formulation after bariatric surgery. Currently no consensus guidelines are available regarding considerations of pharmacotherapy post bariatric surgery. Evidence based national guidelines are warranted as bariatric surgery is becoming a more popular method for the treatment of obesity [44].

Oral drug exposure following bariatric surgery

Reviewing current data on changes in drug exposure prior to and post bariatric surgery reveals many uncertainties regarding the prediction of post bariatric surgery drug bioavailability and the mechanisms behind these changes. BCS did not prove to be enough to explain the observed trend.

Post bariatric surgery imposed restrictions on gastric volume (e.g. SG and RYGB) has been observed to reduce the gastric emptying time of liquids [45, 46] and may further lead to an increase in gastric pH [47, 48]. This together with a reduced fluid intake may impact on the solubility of orally administered drugs.

Statistical analysis did not present any significant trends when examining BCS class I-IV, Do or elimination subgroups. None of the $Do > 1$ classified drugs displayed an increase in bioavailability postoperatively, whereas the $Do \leq 1$ group exhibited a larger variability in pre/post surgery drug exposure outcome. This may be due to solubility issues of the $Do > 1$ group, resulting in an overall reduction in oral drug exposure following surgery. The impact is however unclear due to a low number of drugs falling into the $Do > 1$ category, where further clinical data are necessary to establish the case.

Due to the restriction of the gastric volume following certain types of bariatric surgery (e.g. RYGB and BPD-DS) the default concomitant fluid intake of 250 ml in the BCS may no longer be valid. This will have implications for shifting the boundaries between BCS class I/III and II/IV, such that some freely soluble drugs may become solubility limited dependent on the administered dose. This is further complicated by a potentially altered gastric pH [11, 12, 29, 47, 48].

A small intestinal bypass will reduce the absorption area and may also alter the regional distribution and abundance of drug metabolizing enzymes and transporters thus altering exposure of substrate drugs. When examining drugs with respect to the main route of elimination, no significant difference was observed between CYP3A,

CYP2C, renal and other drugs. These results were also associated with a high degree of uncertainty due to scarcity of data, albeit a higher ppR of CYP3A may be expected due to the GI abundance of CYP enzymes where CYP3A4 is the most highly abundant. The bypass of highly abundant regions of CYP3A4 may lead to an increase in oral bioavailability while such an effect may become less relevant for substrates due to decreasingly abundant CYP2C9/19 and CYP2D6. Such a hypothesis may be supported by the observed trend in AUC of atorvastatin acid, mainly metabolized by CYP3A4 [49], thus potentially displaying an increase in bioavailability post malabsorptive bariatric surgery due to the bypass of significant segments of GI regions highly abundant in CYP3A4 [26], whereas this effect may be counteracted by a reduced absorption area. Following BPD-DS a significant increase in AUC of atorvastatin acid (two-fold) was observed, whereas no significant change was observed following RYGB, thus potentially increasing the risk of adverse effects, such as myopathy, following BPD-DS [36, 37, 50].

The lack of quantifiable drug exposure data means that drugs displaying a low f_g or limited absorption prior to surgery are likely to be wrongly classified when trying to generalize over a wide variety of drugs, such as metformin and phenoxymethylpenicillin.

Metformin, a highly soluble and permeability limited basic compound [51, 52], has been suggested to be subject to saturable transporter uptake to some extent by organic cation transporters in the intestine although this is not fully understood, thus resulting in a dose-dependent absorption that is mainly renally-cleared [53, 54]. The observed increase in postoperative bioavailability [55] might be due to altered small intestinal transit; reductions in gastric emptying time and small intestinal motility would in theory lead to a longer exposure time to enterocytic influx transporters. A further reason could be a post surgical alteration in transporter distribution patterns.

Phenoxymethylpenicillin, considered a highly soluble and permeable compound [52], displayed a significant increase in AUC post JIB, possibly due to a reduced intestinal degradation by bacterial β -lactamase due to a major small intestinal restriction [56].

The different surgical implications on GI physiology may result in variable trends in post surgery drug exposure across the range of bariatric procedures, as is the case with atorvastatin acid displaying a significant increase in AUC following the BPD-DS procedure as compared with no significant change following the less malabsorptive RYGB procedure [36, 37]. Also ciclosporin, there was a reduction in drug exposure following JIB, an exclusively malabsorptive procedure [57, 58], as compared with remaining unaltered following the restrictive AGB [59].

The outcomes of oral drug exposure of many commonly prescribed drugs in bariatric surgery populations are still unknown, such as many antidepressants and analgesics. Current available clinical data are very valuable.

Going forward it is important that further clinical studies are designed taking into consideration the potential alterations in concentration–time profiles, relating to pharmacokinetic parameters such as t_{\max} . Drugs exhibiting a narrow therapeutic range or displaying less readily measurable clinical endpoints will require more stringent monitoring after bariatric surgery, such as immunosuppressant agents and CNS active drugs.

Due to the multiple physiological factors altered in bariatric surgery (i.e. gastric volume, absorption area, CYP-abundance and regional distribution) [11, 12], and the fact that various drugs might be affected to different degrees by each of these changes, physiologically-based pharmacokinetic (PBPK) modelling may help in elucidating the impact of various bariatric surgeries on different drugs given at different doses. Such an investigation was outside the scope of the current research. However initial attempts on this approach are addressed in another report (Darwich *et al.* submitted and under review) where the complex nature of interplays were manifested.

In conclusion, based on current findings, analysis of general pharmacokinetic parameters alone (i.e. solubility, permeability and main route of elimination) is not enough to explain observed trends in oral drug bioavailability following bariatric surgery, although the findings of this study suggest solubility to potentially play an important role.

These implications support the hypothesis that there are several physiologic and drug-specific parameters which govern the observed changes in drug exposure, thus calling for a more mechanistic approach, integrating all known parameters.

To the authors' knowledge this is the first publication quantitatively examining oral drug bioavailability in relation to a set of pharmacokinetic, biopharmaceutic and other drug-specific parameters and also in the context of pharmacotherapeutic practice following bariatric surgery. Along with further clinical studies, PBPK modelling may provide essential insights into the significance of individual pharmacokinetic parameters and generate important clinical guidance for a constantly growing post bariatric surgery population. Currently, there seems to be no simple algorithm or decision tree that predicts the variable changes to drug bioavailability following bariatric surgery.

Competing Interests

There are no competing interests to declare.

Appendix

Table A1

Controlled trials examining oral drug bioavailability following bariatric surgery

Drug	Surgical procedure	Post/pre surgery drug exposure ratio (mean (95% CI))	Additional information	References
Antimicrobials				
Erythromycin 250 mg	GBP	AUC: 0.61 (0.38, 0.99) ($P > 0.05$)*	Controlled prospective study (n patients = 7)	[92]
Ampicillin (pivampicillin 750 mg)	JIB	F_{oral}0.37 (0.16, 0.89) ($P < 0.05$)*	Controlled prospective study (n patients = 6)	[90]
Sulfisoxazole 1000 mg	JIB	F_{oral}: 0.84 (0.74, 0.94) ($P < 0.05$)†	Controlled prospective study (n patients = 3)	[93]
Phenoxymethyl penicillin 1000 mg	JIB	AUC: 10.43 (0.10, 1058) ($P < 0.05$)†	Controlled prospective study (n patients = 3)	[34]
Cardiovascular drugs				
Digoxin 0.5 mg	JIB	AUC: 0.76 (0.59, 0.97) ($P < 0.05$)*	Controlled study (n patients = 9, n controls = 16)	[38]
Digoxin 0.5 mg daily (First day 1 mg)	JIB	AUC: 0.89 (0.70, 1.14) ($P > 0.05$)*	Controlled prospective study (n pre patients = 5, n post patients = 6)	[39]
Hydrochlorothiazide 75 mg	JIB	AUC: 0.46 (0.33, 0.65) ($P < 0.05$)‡	Controlled study as compared to literature data (n patients = 4, n healthy volunteers = 7)	[98, 99]
Immunosuppressants				
Mycophenolic acid (MPA) 2-1000 mg	RYGB‡	AUC: 0.66 (0.21, 2.06)*	Pilot study as compared to literature data (n patients = 2, 4, 1, n controls =)	[33, 102]
Sirolimus 6 mg		AUC: 0.54 (0.25, 1.17)*		
Tacrolimus 2-4 mg		AUC: ‘Reduced’		
Antiepileptics				
Phenytoin 200 mg	JIB	AUC: 0.32 (0.17, 0.58) ($P < 0.05$)*	Controlled study (n patients = 7, n controls = 9)	[101]
Analgesics				
Paracetamol 1500 mg	JIB	AUC: 1.00 (0.647, 1.54) ($P > 0.05$)†	Controlled prospective study (n patients = 3 at 2.7–3.9 months, 5 at 6.4–34 months)	[34]
Phenazone 15 mg kg ^{−1}	JIB	AUC§: 1.06 (0.81, 1.38) ($P > 0.05$)¶	Controlled study (n patients = 17, n controls = 11)	[91]
Oral contraceptives				
Norethisterone 3 mg Levonorgestrel 0.25 mg	JIB	AUC§: 0.80 (0.39, 1.63) ($P < 0.05$)¶ AUC§: 0.55 (0.34, 0.90) ($P < 0.05$)¶	Controlled study (n patients = 6, n controls = 5)	[94]
Estradiol 4 mg Levonorgestrel 0.125 mg	JIB	‘Unaltered’ ‘Unaltered’	Controlled study (n patients = 12)	[103]
‘Contraceptives’	BPD	‘Reduced’	Observed increase in levels of sex-hormone-binding globulin and reduced levels of dehydroepiandrosterone sulphate. Controlled prospective study (n patients = 40)	[104]
Anti-ulceratives				
Ranitidine 300 mg	BPD	AUC: 1.43 (1.12, 1.81) ($P < 0.05$)†	Controlled study (n patients = 11, n controls = 10)	[40]
Ranitidine 150 and 300 mg	BPD	‘Unaltered’	Controlled study as compared to literature data (n patients = 7)	[41]
Statins				
Atorvastatin acid 20–80 mg	BPD-DS	AUC: 1.85 (0.81, 4.27) ($P < 0.05$)*	Controlled prospective study C_{max} ratio: 2.2 ± 1.7 , t_{max} ratio: 2.3 ± 1.3 (n patients = 10)	[36]
Atorvastatin acid 20–80 mg	RYGB	AUC: 1.43 (1.12, 1.81) ($P > 0.05$)*	Controlled prospective study C_{max} ratio: 1.1, t_{max} ratio: 0.5 (n patients = 12)	[37]
Anti-diabetics				
Metformin 1000 mg	RYGB	AUC: 1.20 (0.91, 1.58) ($P > 0.05$)*	Controlled study (n patients = 16, n controls = 16)	[55]
Antidepressants				
Sertraline 100 mg	RYGB	AUC: 0.40 (0.19, 0.84) ($P < 0.05$)*	Controlled study (n patients = 5, n controls = 5)	[100]
Thyroid blockers				
Propylthiouracil 400 mg	JIB	F_{oral}: 1.09 (0.84, 1.42) ($P > 0.05$)*	Controlled prospective study (n patients = 9)	Kampmann 1984

SD, Standard deviation; GBP, Gastric bypass (gastroplasty and Roux-en-Y gastric bypass); JIB, Jejunoileal bypass; BPD, Biliopancreatic diversion; BPD-DS, Biliopancreatic diversion with a duodenal switch; RYGB, Roux-en-Y gastric bypass; AUC, area under curve; F , bioavailability; SS, mean concentration at steady-state; C_{max} , maximum concentration; t_{max} , time at maximum concentration. *Statistical outcome as reported in publication. † t -test performed at 5% significance level. ‡Pre (sirolimus) and post (tacrolimus and MPA) renal transplant patients. §Welch's t -test at a 5% significance level. ¶Calculated estimate of AUC from report.

Table A2Case reports (n patients = 1) on oral drug bioavailability following bariatric surgery

Drug	Surgical procedure	Post/pre surgery drug exposure ratio	Additional information	References
Antimicrobials				
Rifampicin	JIB	Reduced	Following JIB, the rifampicin dose was increased from 600 to 1200 mg in order to reach necessary serum concentrations.	[105]
Isoniazid		Unaltered		
Ethambutol		Unaltered		
Rifampicin	JIB	Reduced	Patient 1: Isoniazid 300 mg – Serum concentration of $3.6 \mu\text{g ml}^{-1}$ at 2 h as compared with reference value of $4\text{--}6 \mu\text{g ml}^{-1}$.	[106]
Isoniazid		Inconclusive	Patient 2: Isoniazid 300 mg – Serum concentration of $8.4 \mu\text{g ml}^{-1}$ at 2 h. Ethambutol 2400 mg – Serum concentration under $1 \mu\text{g ml}^{-1}$. Rifampicin 600 mg – Serum concentration of $4 \mu\text{g ml}^{-1}$ at 4 h as compared with reference value of $8 \mu\text{g ml}^{-1}$.	
Ethambutol		Unaltered		
Rifampicin	JIB	Reduced	Four female patients out of one hundred patients undergoing JIB developed tuberculosis.	[107]
Isoniazid		Unaltered	Blood concentrations were obtained from two patients, displaying a reduced concentration of rifampicin, whereas isoniazid and ethambutol remained within therapeutic range (n patients = 4).	
Ethambutol		Unaltered		
Isoniazid	JIB	Unaltered	Isoniazid and ethambutol blood concentration reported to be within the normal range.	[108]
Ethambutol		Unaltered		
Isoniazid	JIB	Reduced	Drugs excreted in faeces as unaltered tablets after oral administration.	[109]
Ethambutol		Reduced		
Para-aminosalicylic acid		Reduced		
Isoniazid	JIB	Unaltered	Serum concentrations equivalent to that observed in healthy volunteers.	[110]
Ethambutol		Unaltered		
Nitrofurantoin	RYGB	Reduced	Intravenous antibiotics administered due to failure of oral drug therapy failed.	[111]
Amoxicillin		Reduced		
Immunosuppressants				
Tacrolimus	JIB R	AUC: 0.53	After JIB R a 1.90-fold increase in AUC was observed.	[112]
Ciclosporin	JIB	SS concentration: 0.41	n patients = 1, as compared with n controls = 6	[57]
Ciclosporin	JIB R	F_{oral}: 0.36	2.78-fold Increase in drug exposure following JIB R.	[58]
Ciclosporin	LAGBD	Unaltered	Standard cyclosporine therapy was successful in the treatment of a post LAGB surgery patient subject to heart transplant.	[59]
Anticonvulsants				
Phenytoin	RYGB	Reduced	Dose strength up to 500 mg did not achieve therapeutic effect ($<3 \text{ mg l}^{-1}$ as compared with a normal range of $10\text{--}20 \text{ mg l}^{-1}$).	[113]
Phenobarbitone	RYGB	Reduced	At a dose of 60 mg bid, serum levels were reduced (9.9 mg l^{-1}) as compared with normal range ($15\text{--}41 \text{ mg l}^{-1}$).	
Phenytoin	JIB	Reduced	Dose increased from 300 to 500 mg in order to achieve therapeutic effect.	[114]
Ethosuximide	JIB	Reduced	Dose doubled in order to achieve therapeutic effect.	
Phenytoin	JIB R	SS concentration: 0.48	JIB R resulted in an increase in SS concentration.	[115]
Antipsychotics				
Haloperidol	RYGB	Unaltered	Dose doubled immediate post surgery to thereafter be lower to pre surgery dose with effective treatment.	[32]
Anti-cancer drugs				
Imatinib mesylate	BPD-DS	SS concentration: 0.17	Plasma concentration of imatinib 400 mg at steady-state reduced from 965 to 166 ng ml^{-1} .	[35]
Tamoxifen	RYGB	Reduced	3 case reports (n patients = 3).	[116]
Temozolomide	RYGB	AUC: 1.02	Unaltered drug exposure following surgery at a dose of 190 mg as compared with literature.	[117]
Anti-HIV drugs				
Lopinavir/ritonavir	RYGB*	Increased	An observed increase in plasma concentration in comparison with control patients.	[118]
Thyroid hormones				
Thyroxine	JIB	Reduced	Dose increase required from 0.2 mg to 0.8 mg daily to produce sufficient response.	[119]
Thyroxine	JIB	Reduced	C_{max} ratio: 0.31. JIB R restored to pre surgery drug exposure.	[120]
Thyroxine	JIB R	Reduced	Dose increase required from 0.3 mg to 0.6 mg daily to reach SS sufficient concentration.	[121]

JIB, Jejunioleal bypass; JIB R, Jejunioleal bypass reversal; BPD, Biliopancreatic diversion; BPD-DS, Biliopancreatic diversion with a duodenal switch; RYGB, Roux-en-Y gastric bypass; LAGBD, Laparoscopic adjustable gastric banding; AUC, area under curve; F , bioavailability; SS concentration, mean concentration at steady-state; C_{max} , maximum concentration; t_{max} , time at maximum concentration. *Total gastrectomy followed by an oesophagojejunostomy with a Roux-en-Y reconstruction.

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8.1.2 Investigating changes in pharmacotherapy post bariatric surgery: Study protocol and data collection form

Introduction:

The prevalence of obesity has dramatically increased over the last decade. In the USA, where the highest reported obesity rate in the world has been observed, approximately 32.2% of the male and 35.5% of the female population aged 20 years or older were characterised as obese in 2007-2008 (Flegal *et al.*, 2010).

Obesity corresponds with an increased risk for comorbidities, such as cardiovascular diseases and diabetes; subsequently new clinical treatment methods of obesity have therefore emerged during the last decades as the prevalence of obesity has increased. Bariatric surgery, resulting in the removing of parts of the GI tract, has proven to be a clinically and cost effective method of reducing obesity (Picot *et al.*, 2009). These new surgical methods impose new challenges in terms of estimating the pharmacokinetics of orally administered drugs (WHO, 2006; OHE, 2010).

Aim:

This study aims to perform a service evaluation of clinical pharmaceutical practice regarding gastric bypass patient pharmacotherapy pre and post bariatric surgery in an attempt to identify drugs that impose formulation and dose adjustment challenges in post bariatric surgery patients, and additionally identify the required pharmacotherapeutic interventions to meet the patient group's specific treatment needs. This service evaluation is a continuation of a systematic review examining trends in drug absorption after bariatric surgery. In the long term these findings will serve as a substratum for research into predicting and extracting clinical guidance for drug therapy of post bariatric surgery patients.

Personnel:

Personnel that are going to carry out research through the NHS' electronic chart system are undertaking the Master of Science programme in pharmacy at University of Manchester. Additionally personnel have undertaken and passed a Criminal Records

Bureau (CRB) check in accordance with NHS policy. In hospital training will be provided at the IT department at the Royal Salford Hospital in order to be able to utilise and search through the electronic clinical chart system.

Data collection procedure:

The data will be collected through observing the pharmaceutical interventions carried out by clinical pharmacists in practice at a daily basis. The extraction and documentation of information will be done in accordance to the data collection form.

Data analysis:

Acquired data will be analysed through the comparison drug therapy post surgery as compared to pre surgery to identify the most commonly prescribed drugs in bariatric surgery patient groups and to identify systematic changes in. Observed changes will be analysed statistically. The implications of these changes in terms of relations to physiological changes and the impact of change in treatment would further be evaluated.

Data collection form

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Salford Royal Hospital, Salford, UK.

Date of data extraction (DD/MM/YYYY): ____/____/____

Study subject number:

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Type of surgery:

Pre surgery drug therapy

Date (DD/MM/YYYY):

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Days pre bariatric surgery:

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Table 1. Pre surgery drug therapy.

Drug	Administration form	Dosing (mg-times daily)

Comments regarding pharmacotherapy: (underlying comorbidities)

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Post surgery

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Date (DD/MM/YYYY): ____/____/____

Days since bariatric surgery: _____

Table 1. Post surgery drug therapy.

Drug	Administration form	Dosing (mg·times daily)

Reasoning behind drug therapy interventions: (changes in dose, administration form, eventual time period until drug is changed back to original administration form, reason for changes in pharmacotherapy)

8.1.3 Supplementary data on oral drug exposure post bariatric surgery

Table 8.1. Controlled trials examining oral drug exposure following bariatric surgery.

Drug	Surgical procedure	Post/pre surgery drug exposure ratio (mean (CI))	Additional information	References
Antimicrobial drugs				
Erythromycin 250 mg	GBP	AUC: 0.61 (0.38-0.99) ($P>0.05$) ^A	Controlled prospective study (n patients=7)	(Prince <i>et al.</i> , 1984)
Ampicillin (pivampicillin 750 mg)	JIB	F _{oral} : 0.37 (0.16-0.89) ($P<0.05$) ^A	Controlled prospective study (n patients=6)	(Kampmann <i>et al.</i> , 1984)
Sulfisoxazole 1,000 mg	JIB	F _{oral} : 0.84 (0.74-0.94) ($P<0.05$) ^B	Controlled prospective study (n patients=3)	(Garrett <i>et al.</i> , 1981)
Phenoxymethyl penicillin 1,000 mg	JIB	AUC: 10.43 (0.10-1058) ($P<0.05$) ^B	Controlled prospective study (n patients=3)	(Terry <i>et al.</i> , 1982)
Cardiovascular drugs				
Digoxin 0.5 mg	JIB	AUC: 0.76 (0.59-0.97) ($P<0.05$) ^A	Controlled study (n patients=9, n controls=16)	(Gerson <i>et al.</i> , 1980)
Digoxin 0.5 mg daily (First day: 1 mg)	JIB	AUC: 0.89 (0.70-1.14) ($P>0.05$) ^A	Controlled prospective study (n pre patients=5, n post patients=6)	(Marcus <i>et al.</i> , 1977)
Hydrochlorothiazide 75 mg	JIB	AUC: 0.46 (0.33-0.65) ($P<0.05$) ^C	Controlled study as compared to literature data (n patients=4, n healthy volunteers=7)	(Beermann and Groschinsky-Grind, 1977; Backman <i>et al.</i> , 1979)
Immunosuppressants				
Mycophenolic acid (MPA) 2·1,000 mg	RYGB ^C	AUC: 0.66 (0.21-2.06) ^A	Pilot study as compared to literature data (n patients=2, 4, 1, n controls=)	(Dowell <i>et al.</i> , 2007; Rogers <i>et al.</i> , 2008)
Sirolimus 6 mg		AUC: 0.54 (0.25-1.17) ^A		
Tacrolimus 2·4 mg		AUC: 'Reduced'		
Antiepileptic drugs				
Phenytoin 200 mg	JIB	AUC: 0.32 (0.17-0.58) ($P<0.05$) ^A	Controlled study (n patients=7, n controls=9)	(Kennedy and Wade, 1979)

SD=Standard deviation, GBP=Gastric Bypass (gastroplasty and Roux-en-Y gastric bypass), JIB=Jejunioleal Bypass, BPD=Biliopancreatic Diversion, BPD-DS=Biliopancreatic Diversion with a Duodenal Switch, RYGB=Roux-en-Y Gastric Bypass, AUC=Area Under Curve, F=Bioavailability, SS=Mean concentration at steady state, C_{max}=Maximum concentration, t_{max}=Time at maximum concentration. ^AStatistical outcome as reported in publication. ^Bt-test performed at 5% significance level. ^CPre (sirolimus) and post (tacrolimus and MPA) renal transplant patients. ^FCalculated estimate of AUC from report. ^EWelch's t-test at a 5% significance level.

Table 8.1. (Continued) Controlled trials examining oral drug exposure following bariatric surgery.

Drug	Surgical procedure	Post/pre surgery drug exposure ratio (mean (CI))	Additional information	References
Analgesics				
Paracetamol 1,500 mg	JIB	AUC: 1.00 (0.647-1.54) ($P>0.05$) ^B	Controlled prospective study (n patients=3 at 2.7-3.9 months, 5 at 6.4-34 months)	(Terry <i>et al.</i> , 1982)
Phenazone 15 mg/kg	JIB	AUC ^E : 1.06 (0.81-1.38) ($P>0.05$) ^F	Controlled study (n patients=17, n controls=11)	(Andreasen <i>et al.</i> , 1977)
Oral contraceptives				
Norethisterone 3 mg	JIB	AUC ^E : 0.80 (0.39-1.63) ($P<0.05$) ^F	Controlled study (n patients=6, n controls=5)	(Victor <i>et al.</i> , 1987)
Levonorgestrel 0.25 mg		AUC ^E : 0.55 (0.34-0.90) ($P<0.05$) ^F		
Estradiol 4 mg	JIB	'Unaltered'	Controlled study (n patients=12)	(Andersen <i>et al.</i> , 1982)
Levonorgestrel 0.125 mg		'Unaltered'		
'Contraceptives'	BPD	'Reduced'	Observed increase in levels of sex-hormone-binding globulin and reduced levels of dehydroepiandrosterone sulphate. Controlled prospective study (n patients=40)	(Gerrits <i>et al.</i> , 2003)
Anti-ulcerative drugs				
Ranitidine 300 mg	BPD	AUC: 1.43 (1.12-1.81) ($P<0.05$) ^B	Controlled study (n patients=11, n controls=10)	(Cossu <i>et al.</i> , 1999)
Ranitidine 150 and 300 mg	BPD	'Unaltered'	Controlled study as compared to literature data (n patients=7)	(Adami <i>et al.</i> , 1991)
HMG-CoA reductase inhibitors				
Atorvastatin acid 20-80 mg	BPD-DS	AUC: 1.85 (0.81-4.27) ($P<0.05$) ^A	Controlled prospective study C _{max} ratio: 2.2±1.7, t _{max} ratio: 2.3±1.3 (n patients=10)	(Skottheim <i>et al.</i> , 2010)
Atorvastatin acid 20-80 mg	RYGB	AUC: 1.43 (1.12-1.81) ($P>0.05$) ^A	Controlled prospective study C _{max} ratio: 1.1, t _{max} ratio: 0.5 (n patients=12)	(Skottheim <i>et al.</i> , 2009)
Anti-diabetic drugs				
Metformin 1,000 mg	RYGB	AUC: 1.20 (0.91-1.58) ($P>0.05$) ^A	Controlled study (n patients=16, n controls=16)	(Padwal <i>et al.</i> , 2011)
Antidepressants				
Sertraline 100 mg	RYGB	AUC: 0.40 (0.19-0.84) ($P<0.05$) ^A	Controlled study (n patients=5, n controls=5)	(Roerig <i>et al.</i> , 2012)
Thyroid blockers				
Propylthiouracil 400 mg	JIB	F _{oral} : 1.09 (0.84-1.42) ($P>0.05$) ^A	Controlled prospective study (n patients=9)	(Kampman <i>et al.</i> , 1984)

SD=Standard deviation, GBP=Gastric Bypass (gastroplasty and Roux-en-Y gastric bypass), JIB=Jejunioileal Bypass, BPD=Biliopancreatic Diversion, BPD-DS=Biliopancreatic Diversion with a Duodenal Switch, RYGB=Roux-en-Y Gastric Bypass, AUC=Area Under Curve, F=Bioavailability, SS=Mean concentration at steady state, C_{max}=Maximum concentration, t_{max}=Time at maximum concentration. ^AStatistical outcome as reported in publication. ^Bt-test performed at 5% significance level. ^CPre (sirolimus) and post (tacrolimus and MPA) renal transplant patients. ^FCalculated estimate of AUC from report. ^EWelch's t-test at a 5% significance level.

Table 8.2. Case reports (n patients=1) on oral drug exposure following bariatric surgery.

Drug	Surgical procedure	Post/pre surgery drug exposure ratio	Additional information	References
Antimicrobial drugs				
Rifampicin Isoniazid Ethambutol	JIB	‘Reduced’ ‘Unaltered’ ‘Unaltered’	Following JIB, the rifampicin dose was increased from 600 to 1,200 mg in order to reach necessary serum levels.	(Griffiths <i>et al.</i> , 1982)
Rifampicin Isoniazid Ethambutol	JIB	‘Reduced’ ‘Inconclusive’ ‘Unaltered’	Patient 1: Isoniazid 300 mg – Serum concentration of 3.6 µg/mL at 2 hours as compared to reference value of 4-6 µg/mL. Patient 2: Isoniazid 300 mg – Serum concentration of 8.4 µg/mL at 2 hours. Ethambutol 2,400 mg - Serum concentration under 1 µg/mL. Rifampicin 600 mg – Serum concentration of 4 µg/mL at 4 hours as compared to reference value of 8 µg/mL.	(Harris and Wasson, 1977)
Rifampicin Isoniazid Ethambutol	JIB	‘Reduced’ ‘Unaltered’ ‘Unaltered’	Four female patients out of one hundred patients undergoing JIB developed tuberculosis. Blood levels were obtained from two patients, displaying a reduced level of rifampicin, whereas isoniazid and ethambutol remained within therapeutic range (n patients=4).	(Bruce and Wise, 1977)
Isoniazid Ethambutol	JIB	‘Unaltered’ ‘Unaltered’	Isoniazid and ethambutol blood levels reported to be within normal range.	(Pickleman <i>et al.</i> , 1975)
Isoniazid Ethambutol Para-aminosalicylic acid	JIB	‘Reduced’ ‘Reduced’ ‘Reduced’	Drugs excreted in faeces as unaltered tablets after oral administration.	(Werbin, 1981)
Isoniazid Ethambutol	JIB	‘Unaltered’ ‘Unaltered’	Serum levels equivalent to that observed in healthy volunteers.	(Polk <i>et al.</i> , 1978)
Nitrofurantoin Amoxicillin	RYGB	‘Reduced’ ‘Reduced’	Intravenous antibiotics administered due to failure of oral drug therapy failed.	(Magee <i>et al.</i> , 2007)
Immunosuppressants				
Tacrolimus	JIB R	AUC: 0.53	After JIB R a 1.90-fold increase in AUC was observed.	(Kelley <i>et al.</i> , 2005)
Cyclosporine	JIB	SS conc: 0.41	n patients=1, as compared to n controls=6	(Chenhsu <i>et al.</i> , 2003)
Cyclosporine	JIB R	F _{oral} : 0.36	2.78-fold Increase in drug exposure following JIB R.	(Knight <i>et al.</i> , 1988)
Cyclosporine	LAGBD	‘Unaltered’	Standard cyclosporine therapy was successful in the treatment of a post LAGB surgery patient subject to heart transplant.	(Ablassmaier <i>et al.</i> , 2002)

JIB=Jejunioleal Bypass, JIB R=Jejunioleal Bypass Reversal, BPD=Biliopancreatic Diversion, BPD-DS=Biliopancreatic Diversion with a Duodenal Switch, RYGB=Roux-en-Y Gastric Bypass, LAGBD=Laparoscopic Adjustable Gastric Banding, AUC=Area Under Curve, F=Bioavailability, SS Conc=Mean concentration at steady state, C_{max}=Maximum concentration, t_{max}=Time at maximum concentration. ^ATotal gastrectomy followed by an oesophagojejunostomy with a Roux-en-y reconstruction.

Table 8.2. (Continued) Case reports (n patients=1) on oral drug exposure following bariatric surgery.

Drug	Surgical procedure	Post/pre surgery drug exposure ratio	Additional information	References
Anticonvulsants				
Phenytoin	RYGB	‘Reduced’	Dose strength up to 500 mg did not achieve therapeutic effect (<3 mg/l as compared to a normal range of 10-20 mg/l).	(Pournaras <i>et al.</i>)
Phenobarbitone	RYGB	‘Reduced’	At a dose of 60 mg bid, serum levels were reduced (9.9 mg/l) as compared to normal range (15-41 mg/l).	
Phenytoin	JIB	‘Reduced’	Dose increased from 300 to 500 mg in order to achieve therapeutic effect.	(Peterson and Zweig, 1974)
Ethosuximide	JIB	‘Reduced’	Dose doubled in order to achieve therapeutic effect.	
Phenytoin	JIB R	SS conc: 0.48	JIB R resulted in an increase in SS conc.	(Peterson, 1983)
Antipsychotic drugs				
Haloperidol	RYGB	‘Unaltered’	Dose doubled immediate post surgery to thereafter be lower to pre-surgery dose with effective treatment.	(Fuller <i>et al.</i> , 1986)
Anti-cancer drugs				
Imatinib mesylate	BPD-DS	SS conc: 0.17	Plasma concentration of imatinib 400 mg at steady state reduced from 965 to 166 ng/mL.	(Liu and Artz)
Tamoxifen	RYGB	‘Reduced’	3 case reports (n patients=3).	(Wills <i>et al.</i>)
Temozolomide	RYGB	AUC: 1.02	Unaltered drug exposure following surgery at a dose of 190 mg as compared to literature.	(Park <i>et al.</i> , 2009)
Anti-HIV drugs				
Lopinavir/ritonavir	RYGB ^A	‘Increased’	An observed increase in plasma concentration in comparison to control patients.	(Boffito <i>et al.</i> , 2003)
Thyroid hormones				
Thyroxin	JIB	‘Reduced’	Dose increase required from 0.2 mg to 0.8 mg daily to produce sufficient response.	(Topliss <i>et al.</i> , 1980)
Thyroxin	JIB	‘Reduced’	C _{max} ratio: 0.31. JIB R restored to pre surgery drug exposure.	(Azizi <i>et al.</i> , 1979)
Thyroxin	JIB R	‘Reduced’	Dose increase required from 0.3 mg to 0.6 mg daily to reach SS sufficient concentration.	(Bevan and Munro, 1986)

JIB=Jejunioleal Bypass, JIB R=Jejunioleal Bypass Reversal, BPD=Biliopancreatic Diversion, BPD-DS=Biliopancreatic Diversion with a Duodenal Switch, RYGB=Roux-en-Y Gastric Bypass, LAGBD=Laparoscopic Adjustable Gastric Banding, AUC=Area Under Curve, F=Bioavailability, SS Conc=Mean concentration at steady state, C_{max}=Maximum concentration, t_{max}=Time at maximum concentration. ^ATotal gastrectomy followed by an oesophagojejunostomy with a Roux-en-y reconstruction.

8.1.4 Statistical data analysis

The combined standard deviation (S_{pooled}) was computed utilising Equation 8.1, where S_n denotes the sample standard deviation and n represents the sample size.

$$S_{\text{pooled}} = \sqrt{\frac{(n_1 - 1) \cdot S_1^2 + (n_2 - 1) \cdot S_2^2}{n_1 + n_2 - 2}}$$

Equation 8.1: Pooled variance.

The natural logarithmic ratio ($\ln R$) was computed from sample means (\bar{X}_n ; Equation 8.2):

$$\ln R = \ln(\bar{X}_1) - \ln(\bar{X}_2)$$

Equation 8.2: logarithmic ratio.

The variance of the log response ratio ($V_{\ln R}$) was obtained through Equation 8.3:

$$V_{\ln R} = S_{\text{pooled}}^2 \left(\frac{1}{n_1 \cdot (\bar{X}_1)^2} + \frac{1}{n_2 \cdot (\bar{X}_2)^2} \right)$$

Equation 8.3: Variance of ratio.

The standard error of the log response ratio ($SE_{\ln R}$; Equation 8.4) was calculated from the variance:

$$SE_{\ln R} = \sqrt{V_{\ln R}}$$

Equation 8.4: Standard error of ratio.

The log ratio was converted to the geometric mean ratio (R), upper and lower 95th Percentiles (UL_R and LL_R respectively) utilising the exponent (e) utilising Equation 8.5, Equation 8.6 and Equation 8.7:

$$R = e^{\ln R}$$

Equation 8.5: Geometric mean ratio.

$$LL_R = e^{LL_{lnR}}$$

Equation 8.6: Lower percentile of geometric mean ratio.

$$UL_R = e^{UL_{lnR}}$$

Equation 8.7: Upper percentile of geometric mean ratio.

The weighted mean (WX) was calculated based on averages (x_j) and sample sizes (n_j) from literature data (Equation 8.8) (Ghobadi *et al.*, 2011):

$$WX = \frac{\sum_{j=1}^n n_j \cdot x_j}{\sum_{j=1}^n n_j}$$

Equation 8.8: Weighted mean.

Overall sum of squares (SS) was obtained based on standard deviations (SD_j) from literature data, x_j , n_j , overall sample size (N) and WX (Equation 8.9):

$$SS = \sum \left[\{SD_j^2 + x_j^2\} \cdot n_j \right] - N \cdot WX^2$$

Equation 8.9: Overall sum of squares.

Overall SD was obtained from SS and N (Equation 8.10):

$$SD = \sqrt{\frac{SS}{N}}$$

Equation 8.10: Overall standard deviation.

The coefficient of variance (CV) was obtained based on SD and WX (Equation 8.11):

$$CV = \frac{SD}{WX}$$

Equation 8.11: Coefficient of variation.

Overall σ was obtained from the log-transformed CV (Equation 8.12):

$$\sigma = \sqrt{\ln(1 + CV^2)}$$

Equation 8.12: Log-transformed coefficient of variation.

The overall μ was obtained from WX and σ (Equation 8.13):

$$\mu = \ln(WX) - (0.5 \cdot \sigma^2)$$

Equation 8.13: Log-transformed mean ratio.

The overall geometrical mean (GM) was obtained from the exponent of μ (Equation 8.14):

$$GM = e^{\mu}$$

Equation 8.14: Geometric mean.

The overall geometrical standard deviation (GSD) was obtained from the exponent of σ (Equation 8.15):

$$GSD = e^{\sigma}$$

Equation 8.15: Geometric standard deviation.

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8.2 A mechanistic pharmacokinetic model to assess modified oral drug bioavailability post bariatric surgery in morbidly obese patients: interplay between CYP3A gut wall metabolism, permeability and dissolution

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A mechanistic pharmacokinetic model to assess modified oral drug bioavailability post bariatric surgery in morbidly obese patients: interplay between CYP3A gut wall metabolism, permeability and dissolution

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Keywords

ADAM model; bariatric surgery; obesity; oral drug bioavailability; pharmacokinetic modelling

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Abstract

Objectives Due to the multi-factorial physiological implications of bariatric surgery, attempts to explain trends in oral bioavailability following bariatric surgery using singular attributes of drugs or simplified categorisations such as the biopharmaceutics classification system have been unsuccessful. So we have attempted to use mechanistic models to assess changes to bioavailability of model drugs.

Methods Pharmacokinetic post bariatric surgery models were created for Roux-en-Y gastric bypass, biliopancreatic diversion with duodenal switch, sleeve gastrectomy and jejunoileal bypass, through altering the 'Advanced Dissolution Absorption and Metabolism' (ADAM) model incorporated into the Simcyp® Simulator. Post to pre surgical simulations were carried out for five drugs with varying characteristics regarding their gut wall metabolism, dissolution and permeability (simvastatin, omeprazole, diclofenac, fluconazole and ciprofloxacin).

Key findings The trends in oral bioavailability pre to post surgery were found to be dependent on a combination of drug parameters, including solubility, permeability and gastrointestinal metabolism as well as the surgical procedure carried out.

Conclusions In the absence of clinical studies, the ability to project the direction and the magnitude of changes in bioavailability of drug therapy, using evidence-based mechanistic pharmacokinetic *in silico* models would be of significant value in guiding prescribers to make the necessary adjustments to dosage regimens for an increasing population of patients who are undergoing bariatric surgery.

Introduction

The prevalence of obesity has increased dramatically in the USA and Europe over the last decade.^[1–4] Bariatric surgery has proven to be successful in treating morbid obesity. In 2008, approximately 220 000 bariatric surgeries were performed in the USA and Canada, and over 66 000 operations were carried out in Europe.^[5,6]

Several bariatric surgical procedures currently coexist in healthcare, being characterised as either restrictive, in terms of reducing gastric capacity, malabsorptive, with regard to restricting the small intestine and/or delaying the bile inlet, or a combination of both.^[7,8] These procedures include: adjustable gastric band, sleeve gastrectomy, biliopancreatic diversion (BPD), biliopancreatic diversion with a duodenal switch (BPD-DS) and Roux-en-Y gastric bypass (RYGB).^[9] Other procedures, such as jejunoileal bypass, have been gradually

phased out due to a higher likelihood of adverse events (Figure 1).^[4,10,11]

Different types of bariatric surgery will impose a number of physiological changes varying in extent depending on the invasiveness of the procedure. Many of these alterations are known to affect the bioavailability of orally administered drugs, although studies investigating alterations in oral drug exposure pre- to postoperatively have been limited.^[12]

Oral bioavailability (F_{oral}) is dependent on the fraction of drug that is absorbed in the intestinal gut wall (f_a), the fraction that escapes gut wall metabolism (F_G) and the fraction that escapes hepatic metabolism (F_H) (Equation 1).

$$F_{\text{oral}} = f_a \cdot F_G \cdot F_H \quad (1)$$

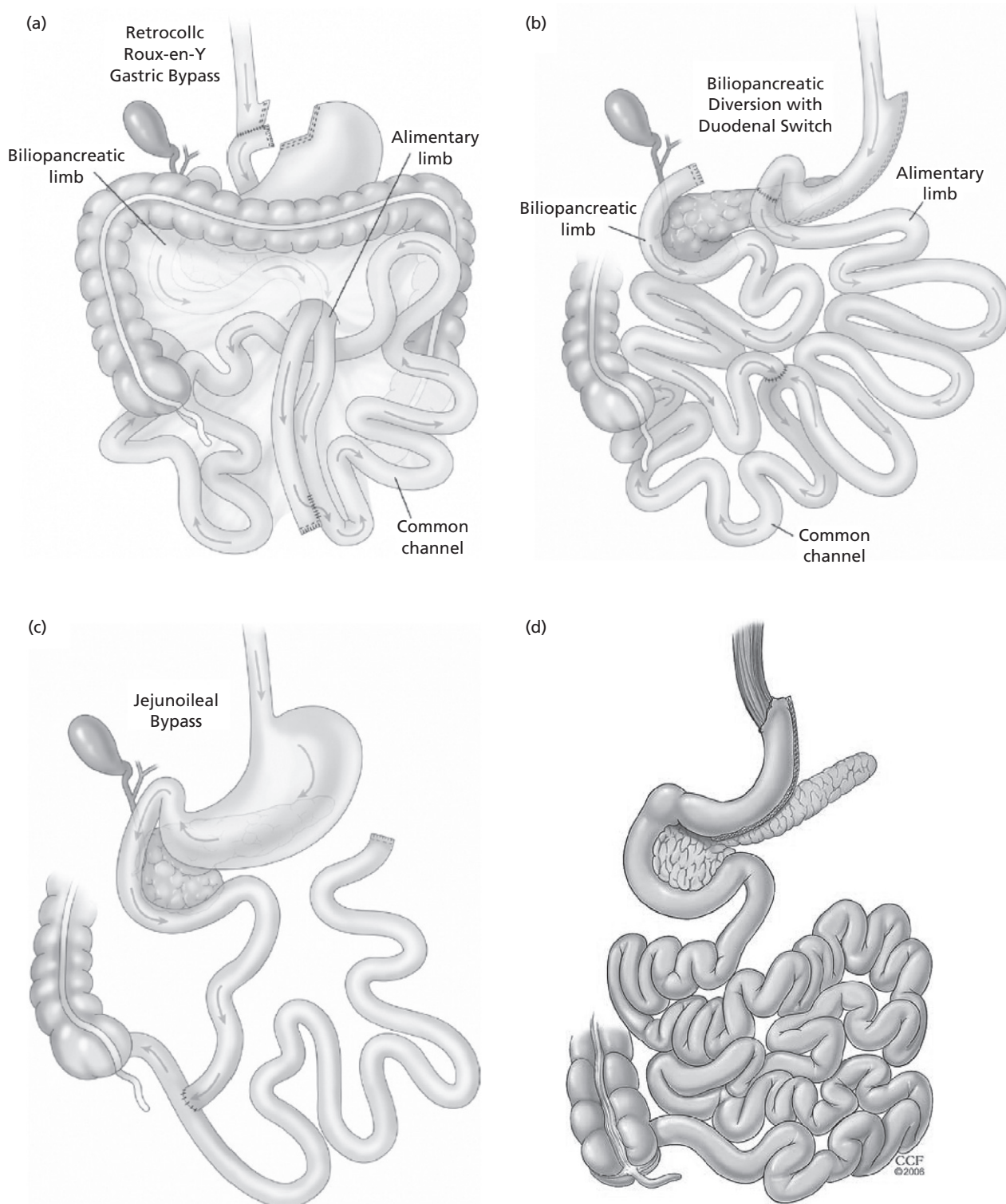


Figure 1 Schematic illustrations of selected bariatric surgical procedures imposing restrictions to the gastrointestinal tract. (a) Roux-en-Y gastric bypass. (b) Biliopancreatic diversion with duodenal switch. (c) Jejunioileal bypass.^[4] (d) Sleeve gastrectomy.^[3]

Both f_a and F_G are highly influenced by drug and formulation properties, such as disintegration, dissolution, permeability, solubility, and the susceptibility to being metabolised by certain enzymes (e.g. certain cytochrome P450 families (CYP3A) or UDP-glucuronosyltransferases). Gastrointestinal (GI) physiology such as gastric emptying time, pH profile, small intestinal transit time, abundance and genotype of gut wall drug metabolising enzymes and transporters can also affect f_a and F_G .^[13,14]

Gastric emptying time can serve as the rate limiting step for highly permeable and highly soluble drugs as the absorption from the stomach is inevitably low.^[15] The gastrointestinal pH may affect drug dissolution for drugs displaying a pK_a within the range of GI pH fluctuations.^[16,17] Furthermore, small intestinal transit time may influence the drug absorption of poorly soluble or extended release drug formulations as it is the main site of absorption.^[18] Metabolism in the gut acts to regulate the oral bioavailability of drugs and other xenobiotics, an important determinant in the metabolism of substrate drugs.^[19] Cytochrome P450 (CYP), UDP-glucuronosyltransferases, sulfotransferases and glutathione S-transferases drug metabolising enzymes are present in the enterocytes along the GI tract. CYP3A4 is the most abundant drug metabolising enzyme in the GI tract, preceding CYP2C9, CYP2C19, CYP2J2 and CYP2D6 in order of abundance.^[20–23] CYP3A4 and CYP3A5 are both present along the whole GI tract, where CYP3A4 is expressed at lower levels in the duodenum, rising in the jejunum and decreasing towards the ileum.^[19,24]

GI transporters may influence the absorption of orally administered drugs and potentially also the extent of metabolism in the gut through active substrate efflux.^[25,26] Numerous transporters are present in the gut, such as the multidrug resistance transporter 1, also referred to as P-glycoprotein (P-gp), multidrug resistance associated protein 2 and breast cancer related protein.^[27,28] P-gp is the most extensively studied of the GI transporters and the relative expression pattern of P-gp in the small intestine increases from the proximal to the distal parts of the small intestine.^[29]

The advanced dissolution absorption and metabolism (ADAM) model is a mechanistic representation of the GI tract which is implemented into the Simcyp Simulator.^[30] It is a successive development of the advanced compartmental absorption and transit model,^[31,32] and includes distinct parameters that better reflect the physiology with regards to handling of fluid dynamics (no constant volume in each segment), anatomical mirroring of the GI anatomy and biology for different segments (unequal segments with relative abundance of enzymes), and dissolution models (avoiding assumptions of a flat surface in Noyes-Whitney). The model defines the amount of drug in 'formulation', 'released but undissolved', 'dissolved' and 'enterocytes' as separate compartment structures and further adds hepa-

tobiliary circulation and bile mediated solubility (Figure 2). The model also incorporates fluid dynamics along the GI tract flowing at the rate of gastric emptying and small intestinal transit time, and rates of fluid absorption, secretion and reabsorption along the GI tract as opposed to a static volume in each segment.^[14]

Furthermore, the ADAM model incorporates the abundance and distribution of GI enzymes and inter-individual variability as well as the distribution of the GI transporter P-gp.^[14] The model attributes can be modified to reflect changes following bariatric surgery in a morbidly obese patient population^[33] and to investigate the validity of predicting the influence of surgery on oral bioavailability of drugs.

Due to the multifactorial physiological implications of bariatric surgery, attempts to explain trends in changes to oral bioavailability following bariatric surgery using single attributes of drugs or simplified categorisations such as the biopharmaceutics classification system (BCS) have been unsuccessful.^[12]

In the absence of clinical studies showing the direction and magnitude of changes in bioavailability of various drugs, evidence-based mechanistic pharmacokinetic in-silico models that define such alterations would be of value in determining appropriate dosage regimens for an increasing patient population undergoing bariatric surgery. The current study, to our knowledge, is the first to develop such a model.

Methods

Characterisation of post bariatric surgery population

A set of gastrointestinal and whole-body physiological parameters were identified based on factors influencing oral drug bioavailability post bariatric surgery. These included: gastric volume and gastric emptying rate, gastrointestinal pH, post surgical small intestinal dimensions, small intestinal motility and transit time, and bile properties. Whole-body physiological factors known to influence oral drug exposure were also identified, such as renal function and serum protein levels as a function of post surgical weight loss.

An extensive literature search of identified parameters in relation to bariatric surgery was performed utilising PubMed (1966–2011). The gastrointestinal and physiological parameters were analysed in accordance with appropriate functions. Weighted means (WX) and standard deviations (overall SD) of results were calculated from the reported means (\bar{x}) and standard deviations (SD), dependent on the number of observations in the i^{th} study (n) (Equations 2, 3 and 4), and where applicable were analysed using Welch's t -test at a significance level of 0.05 assuming parameter data to be normally distributed and taking unequal variance (s) into

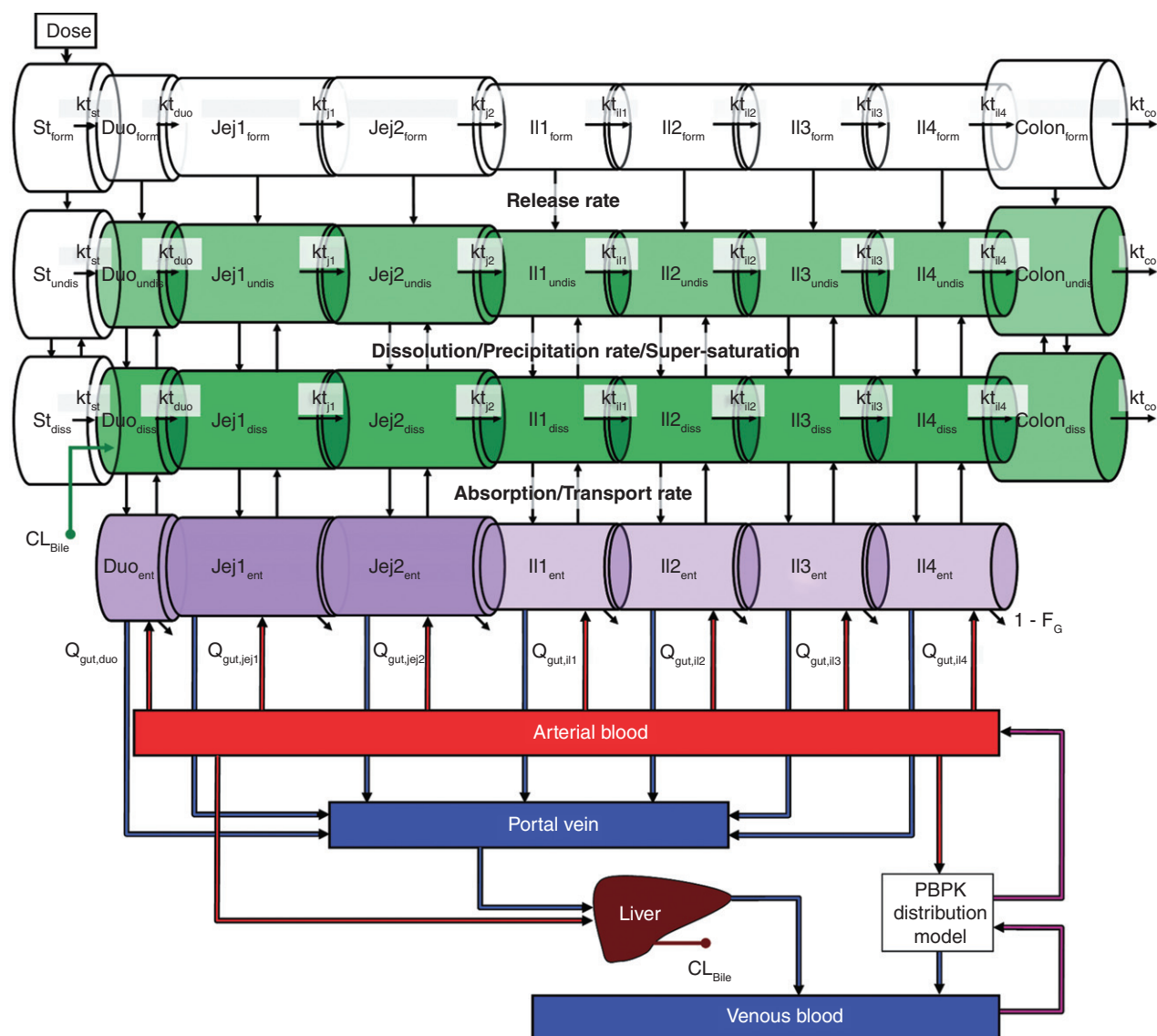


Figure 2 Depiction of the 9-segment ADAM model consisting of the following compartments: stomach, duodenum, jejunum I, jejunum II, ileum I–IV and colon. St, stomach; Jej1 and 2, jejunum; Il1–4, ileum; form, drug trapped in formulation; undiss, undissolved drug; diss, dissolved drug; ent, fraction absorbed drug in enterocytes; k_t , transit rate; Q_{gut} , gastrointestinal blood flow; F_g , fraction drug that escapes gut wall metabolism; CL_{bile} , biliary clearance. Compartment size and purple colour intensity refers to segmental length and regional abundance of CYP3A4 respectively. Green colour scheme indicates bile enhanced solubility. Adapted from Jamei *et al.*^[14]

account, where X is the sample mean and N is the sample size (Equation 5).

$$WX = \frac{\sum_{i=1}^n n_i \cdot x_i}{\sum_{i=1}^n n_i} \quad (2)$$

$$\text{Overall SD} = \sqrt{\frac{\text{Overall sum of squares}}{N}} \quad (3)$$

Overall sum of squares =

$$\sum_{i=1}^n \left[\{(SD_i)^2 + (x_i)^2\} \cdot n_i \right] - N \cdot WX^2 \quad (4)$$

$$t = \frac{X_1 - X_2}{\sqrt{\frac{s_1^2}{N_1} + \frac{s_2^2}{N_2}}} \quad (5)$$

Adapting the ADAM model to mimic post bariatric surgery conditions

The Simcyp Simulator v10 (Simcyp Limited, Sheffield, UK) population template for the morbidly obese based on a northern European Caucasian population was used. Validation of this model with respect to prediction of clearance has recently been published by Ghobadi *et al.*^[33] We re-evaluated and analysed model performance against the identified post bariatric surgery model. Whenever applicable, we altered necessary population parameters to conform to post bariatric surgery conditions, applying reported data of weighted means and coefficient of variation (CV %) (Table 1).

Post bariatric surgery gastrointestinal physiological parameters based on population/surgical data or physiologically rational assumptions were implemented into the ADAM model, creating 'post sleeve gastrectomy', 'post Roux-en-Y gastric bypass', 'post biliopancreatic diversion with duodenal switch' and 'post jejunoileal bypass' population templates (so called population files within Simcyp).

Post surgical basal steady state gastric fluid volumes at fasted state were estimated through one-compartmental simulations of gastric fluid dynamics (Equation 6) in Matlab R2010a (MathWorks, Natick, MA, USA) utilising reported post surgical gastric emptying and assuming a linear relationship with regards to the excretion of gastric juices (0.08 l/h) as a function of gastric capacity, utilising an average gastric volume of 230 ± 13 ml as reported in 134 individuals. Saliva production was kept constant at 0.05 l/h.^[14,34,35] Where V_{st} is the volume of fluids in the stomach, $Q_{sec,st}$ is the secretion of fluids into the stomach, and $k_{t,st}$ is the rate at which the stomach is emptied.

$$\frac{dV_{st}}{dt} = Q_{sec,st} - k_{t,st} V_{st} \quad (6)$$

Table 1 Pre to post surgery physiological parameters evaluated

Gastric emptying of liquids (min)
Gastric emptying of solids (min)
Postoperative gastric volume (ml)
Secretion in stomach (Q_{sec} ; l/h)
Initial volume of stomach fluid (ml)
Small intestinal bypass (cm)
Small intestinal bile delay (cm)
Small intestinal bile concentrations at fasted and fed state (nM)
Gastrointestinal pH at fasted and fed state
Gastrointestinal CYP3A4 abundance (nmol/total gut)
Gastrointestinal CYP3A5 abundance (nmol/total gut)
Small intestinal transit time (h)
Renal function (glomerular filtration rate; ml/min)
Human serum albumin levels (g/l)
α -1 Acid glycoprotein levels (g/l)
Hepatic function (enzymatic activity)

Population implementations of small intestinal bypass and delay in bile inlet were dimensionally estimated as a function of body surface area (BSA) utilising Equations 7 and 8 as implemented into the Simcyp Simulator ADAM model. Further, the human effective permeability (P_{eff}) was set to close to zero in segments corresponding to the small intestinal bypass in the drug template.^[36]

$$\text{Length of duodenum} = 0.205 \cdot BSA^{0.550} \quad (7)$$

$$\text{Length of jejunum and ileum} = 5.231 \cdot BSA^{0.414} \quad (8)$$

Post surgical estimations of small intestinal transit time were implemented into the ADAM model utilising the incorporated Weibull distribution fitted to describe a log normal distribution through altering the scale factor (β) of small intestinal transit time, keeping the shape factor (α) constant, altering β thus retaining the log normal distribution assumption (Equation 9).^[36]

$$f(x) = \frac{\alpha}{\beta} \left(\frac{x}{\beta} \right)^{\alpha-1} e^{-(x/\beta)^\alpha} \quad (9)$$

Following the dimensional alterations to the postoperative surgical GI anatomy, the bariatric surgical team at Salford Royal Foundation NHS Hospital Trust (Salford, UK) was consulted in order to establish consensus on physiological dimensions reflecting a realistic patient population. The parameters subject to a consensus discussion included: post surgical gastric volume and capacity, small intestinal bypass and delay in bile inlet.

Virtual study of bioavailability post bariatric surgery

An identified set of compounds in the Simcyp Simulator were simulated utilising 'post sleeve gastrectomy in morbidly obese', 'post Roux-en-Y gastric bypass in morbidly obese', 'post biliopancreatic diversion with duodenal switch in morbidly obese' and 'post jejunoileal bypass in morbidly obese' population templates in a total of 100 subjects per group, with an age range of 20 to 50 years and 0.50 proportion of females, varying the mean small intestinal transit time to account for any ambiguity in reported data following surgery.

The selected drugs (simvastatin, omeprazole, diclofenac, fluconazole and ciprofloxacin) had a wide range of physicochemical and metabolic attributes and were commonly used in patients undergoing bariatric surgery.^[12] Oral drug exposure was simulated for a low, medium and high therapeutic dose in accordance with the British National Formulary, which included: simvastatin immediate release (10, 20 and 80 mg), diclofenac enteric coated (25, 50 and 75 mg),

omeprazole enteric coated (10, 20 and 40 mg), fluconazole immediate release (50, 200, 400 mg) and ciprofloxacin immediate release (250, 500 and 750 mg). Drugs simulated in post bariatric surgery population templates were compared with simulations carried out in the 'morbidly obese' population template, examining trends in oral drug bioavailability, f_a and F_G (Equation 1), and related surrogate biomarkers: $AUC_{0-24\text{ h}}$, C_{max} and t_{max} where simulated data were processed utilising Matlab R2010a.

Results

Characterisation and validation of virtual populations

Roux-en-Y gastric bypass

Post RYGB stomach volume

A reduced gastric volume was implemented into the 'morbidly obese' population template through limiting concomitant fluid intake from the default value of 250 ml to 30 ml based on surgical restriction in accordance to Wittgrove & Clark.^[37] The initial volume of stomach fluid in the fasted state was estimated to be 9.9 ml (CV 30%) utilising simulations at steady state as per Equation 6.

Gastric acid secretion and pH

Two studies were identified measuring gastric acid production in a total of 18 post RYGB patients, with an approximate gastric volume of 10 ml, as compared with pre surgery or controls.^[38,39] Combining weighted means and variance displayed a mean basal gastric acid excretion of

0.08 ± 0.008 mEq/h, and a weighted mean peak acid excretion of 0.048 ± 0.048 mEq/30 min post surgery, as compared with a basal and peak acid excretion of 9.1 ± 3.6 mEq/h ($P < 0.05$) and 12.8 ± 1.8 mEq/30 min ($P < 0.05$), respectively, in pre surgery patients ($n = 8$), and a basal and peak acid secretion of 5.0 ± 0.7 ($P < 0.05$) and 12.1 ± 1.3 ($P < 0.05$), respectively, in healthy volunteers ($n = 15$)^[38,39] (Figure 3). Implementation into the Simcyp Simulator 'morbidly obese' population template was based on the assumption of gastric pH of 6.4 in the fasted state.

Gastric emptying time

Following RYGB surgery a significant reduction in $t^{1/2}$ gastric emptying time has been observed for liquids, whereas available data on gastric emptying of solids display a considerably increased variability (Figures 4 and 5). Four studies measuring gastric emptying time following gastrectomy surgery were identified (RYGB, sleeve gastrectomy, Billroth gastrectomy with Roux-en-Y gastrectomy and partial gastrectomy). Combining weighted means and variance in a total of 68 post surgery patients resulted in a mean $t^{1/2}$ gastric emptying of 8.48 ± 9.12 min, as compared with 24.33 ± 23.71 min in controls ($n = 39$; $P < 0.05$) (Figure 4).^[40-43]

Identified publications examining gastric emptying time of solids post gastric surgery resulting in a reduced gastric volume (RYGB, sleeve gastrectomy and Billroth gastrectomy with Roux-en-Y gastrectomy) displayed an observable increase in variability following surgery as compared with controls, with reported observations ranging from 4 min to over 200 min post surgery (Figure 5).^[40-46]

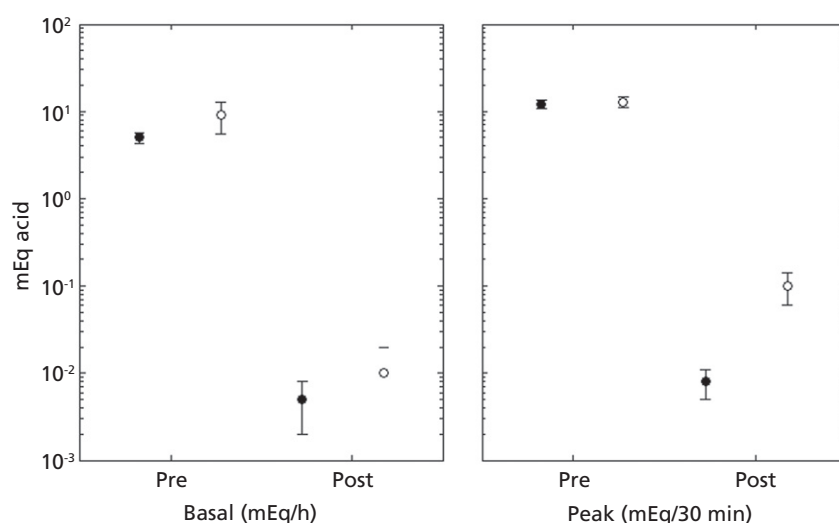


Figure 3 Acid secretion over time at basal and peak levels. Acid secretion (mean \pm SD, mEq HCl) in 12 post Roux-en-Y gastric bypass patients as compared with 15 healthy volunteers not subject to surgery (●).^[38] Acid secretion in eight Roux-en-Y gastric bypass patients, pre and post surgery (○).^[39]

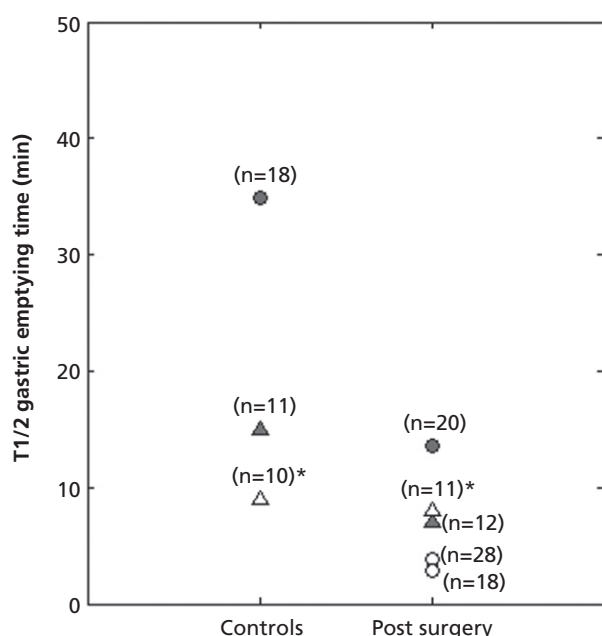


Figure 4 Reported mean (*median) $t_{1/2}$ gastric emptying time of liquids in post gastric surgery patients subject to various surgeries resulting in a reduced gastric volume as compared with controls (pre surgery or healthy volunteers not subject to surgery). (●) Sleeve gastrectomy, (○) Billroth gastrectomy and Roux-en-Y gastrojejunostomy, (▲) Roux-en-Y gastric bypass and (△) Roux-en-Y gastrectomy.^[40–43]

Following RYGB, the gastric emptying half life of liquids was measured to be 7 ± 3 min after liquid intake in 12 post gastric bypass patients 12 months post surgery with a newly formed stomach pouch size of 60–80 ml and a gastrojejunal anastomosis of 12–20 mm in diameter, as compared with 11 healthy volunteers displaying a gastric emptying half life of 15 ± 2 min (Figure 5).^[42]

Gastric emptying half life of a solid meal was highly variable in the post RYGB patient population, where four patients displayed a $t_{1/2}$ of 24 ± 10 min, exhibiting an initial rapid gastric emptying followed by a linear emptying, whereas five patients displayed an initial lag time followed by linear emptying. Three patients displayed a prolonged lag time followed by slow gastric emptying, with a reported gastric emptying half time of over 200 min. The control group displayed a $t_{1/2}$ of 70 ± 7 min (Figure 5).^[42] Alteration of the gastric emptying was implemented based on post surgical gastric emptying time for liquids of 7 min (CV 45%) in the fasted state.^[42]

Small intestinal bypass and regional abundance of CYP3A

Approximately 75–100 cm of the proximal small intestine is bypassed following RYGB surgery, bypassing the duodenum and proximal jejunum.^[4,7,37,47–49] In accordance with the small

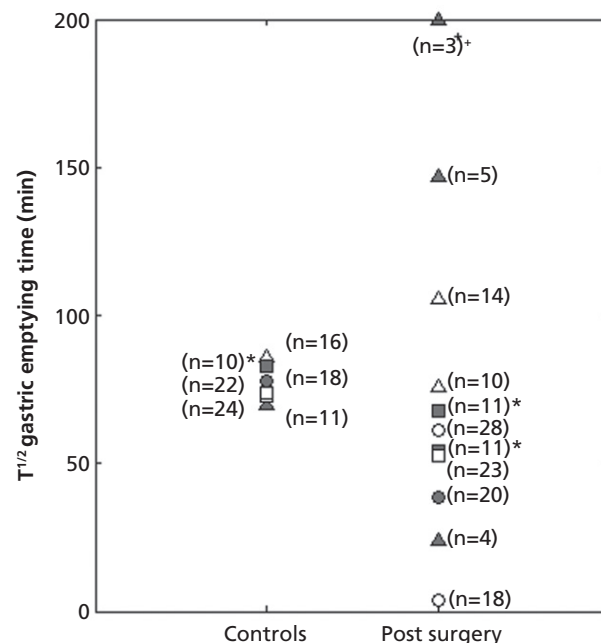


Figure 5 Reported mean (*median) $t_{1/2}$ gastric emptying time of solids in post gastric surgery patients subject to various gastrointestinal surgeries, as described in publication, resulting in a reduced gastric volume as compared with controls. (●) Sleeve gastrectomy, (○) Billroth gastrectomy and Roux-en-Y gastrojejunostomy, (▲) Roux-en-Y gastric bypass, (△) Roux-en-Y gastrectomy, (■) Roux-en-Y gastrectomy, (□) sleeve gastrectomy.^[40–46]

intestinal bypass, the duodenum and proximal jejunum were bypassed through setting transit time close to zero in the duodenum and reducing small intestinal transit time in jejunum I by 38%, thus creating an approximate bypass of 87.5 cm in the ADAM model based on body surface area (Equations 7 and 8).

Small intestinal motility and transit time

Studies in humans examining small intestinal transit and motility in patients subject to total gastrectomy^[50,51,52] were reviewed as compared with a partial gastrectomy in the treatment of obesity.^[37]

The data suggested changes in small intestinal motility after a Roux-en-Y reconstruction.^[52,53] In ten patients subject to Roux-en-Y with a total gastrectomy (cancer being the main indication), a mean small intestinal transit for solids of 293 ± 37 min was observed as compared with 187 ± 37 min in five controls ($P < 0.02$), thus suggesting the small intestinal transit to be increased post RYGB.^[50] Animal models of RYGB surgery suggested a similar impact of surgery as that observed in man, with disturbed small intestinal motility reported in rat and dog.^[54–56]

Two scenarios were created with regards to small intestinal transit time. In the first scenario the transit time was assumed

to be 5.0 h based on a reduced motility as reported by Pellegrini *et al.*^[50] whereas, in the second scenario the small intestinal motility was assumed to remain unaltered, thus reducing small intestinal transit to 3.0 h as a function of the small intestinal bypass.

Regional abundance of CYP3A metabolising enzymes was set to close to zero in the bypassed segments of the small intestine. Mean total enzyme abundance of CYP3A4 and CYP3A5 was recalculated to account for the small intestinal bypass of the duodenum, resulting in a reduction from 66.2 to 50.2 nmol/total gut and from 24.6 to 18.7 nmol/total gut, respectively.^[36]

Bile and pancreatic fluids

Following RYGB surgery, the inlet of bile and pancreatic fluids is delayed to the common channel approximately 75–150 cm distally of the newly formed stomach pouch.^[37,47,48] A delayed bile inlet was implemented into the ADAM model through setting bile concentrations in the fasted and fed state to zero in the gastrointestinal regions of the stomach, duodenum and jejunum corresponding to approximately 90 cm.

Biliopancreatic diversion with duodenal switch

Stomach volume

In accordance with the surgical procedure the gastric volume following biliopancreatic diversion with duodenal switch was effectively restricted to 150 ml through limiting concomitant fluid intake with oral administration to 150 ml. Due to lack of data, gastric emptying and gastric pH was assumed to remain unaltered.^[4,7,37–39,47,48]

Small intestinal bypass and regional abundance of CYP3A

Jejunum segments Jej1 and 2 were bypassed corresponding to approximately 294 cm,^[37] recalculating gastrointestinal abundance of CYP3A4 and CYP3A5 accordingly to 30.0 and 11.2 nmol/total gut respectively.^[36]

Small intestinal motility and transit time

In the first scenario the transit time was assumed to be 3.7 h in accordance with the reduced motility observed post total gastrectomy with Roux-en-Y jejunostomy corrected for the small intestinal length following BPD-DS.^[50] In the second scenario the small intestinal motility was assumed to be 2.2 h, thus reducing as a function of the small intestinal bypass.

Bile and pancreatic fluids

In accordance with the surgical procedure the bile inlet was delayed to ileum III corresponding to 252 cm.^[4,7,37]

Sleeve gastrectomy

Stomach volume

Sleeve gastrectomy surgery is limited to restriction of the dimension of the gastric pouch (to approx. 60–80 ml), preserving the pyloric sphincter.^[8,57] Although not as invasive as malabsorptive procedures, the reduction in gastric volume has been reported to affect the gastric emptying time of liquids and solids (Figures 4 and 5).^[40,44] This was implemented through setting concomitant fluid intake to 80 ml and initial volume of stomach fluid to 24.2 ml (CV: 30%) in the fasted state in accordance with simulated steady state gastric volumes.

Gastric emptying time

One study was identified examining gastric emptying of liquids following sleeve gastrectomy, observing a significantly reduced $t_{1/2}$ gastric emptying time of 13.6 ± 11.9 min in 20 post surgery patients as compared with $34. \pm 24.6$ min in 18 controls (Figure 4).^[40] Thus, gastric emptying was set to 13.6 (CV: 53%) in the post sleeve gastrectomy population template.

Results from combining weighted means and variance of identified studies examining gastric emptying of solids resulted in a significant reduction postoperatively ($P < 0.05$), with an observed mean gastric emptying time of 46.1 ± 17.7 min in 43 post surgery patients as compared with 74.6 ± 26.2 min in 64 controls (Figure 5).^[40, 44]

Gastric acid secretion and pH

There is a lack of published data on the impact of sleeve gastrectomy on gastric acid secretion or gastric pH measurements pre to post surgery. Given this, gastric pH was assumed to remain unaltered following sleeve gastrectomy.

Jejunioileal bypass

Small intestinal bypass and regional abundance of CYP3A

In accordance with the surgical procedure a small intestinal bypass was created retaining the duodenum segment, approximately 20% of the proximal jejunum I and 23% of the terminal ileum IV, bypassing the remainder of the small intestine.^[10,58,59] Accordingly, the abundance of CYP3A4 and CYP3A5 was set to zero in jejunum II to ileum III and recalculated to 32.3 and 12.1 nmol/total gut, respectively.

Small intestinal motility and transit time

In the first scenario the transit time was assumed to be 0.7 h in accordance with the reduced motility observed post total gastrectomy with Roux-en-Y jejunostomy corrected for the small intestinal length post jejunioileal bypass.^[50] In the second scenario the small intestinal motility was assumed to be 0.4 h, thus reducing as a function of the small intestinal bypass.

Bariatric surgery: whole-body physiological parameters

Renal function

Comparing observed data on renal function, in terms of glomerular filtration rate (GFR), in relation to body mass index (BMI) following bariatric surgery induced weight loss, estimates made utilising Cockcroft-Gault and modification of diet in renal disease (MDRD; Equation 10) equations, concluded a better prediction by the MDRD equation.^[60–63] The Cockcroft-Gault equation estimates the creatinine clearance, while the MDRD equation estimates the GFR corrected for body surface area.^[64] Simulating age and sex matched populations over a range of BMI, utilising the Simcyp Simulator incorporating inter-individual variability, observed data was within 95% confidence interval of simulated estimations utilising the MDRD equation, whereas, the Cockcroft-Gault equation over-predicted GFR at a higher BMI in agreement with previous publications examining predicted versus observed GFR in ‘morbidly obese’ and ‘obese’ populations.^[33,63] Based on these findings the MDRD equation was utilised to estimate GFR in the Simcyp Simulator (Figure 6).

$$\text{GFR (mL/min/1.73m}^2\text{)} = \frac{186 \cdot \text{Serum creatinine (mg/dL)}^{-1.154}}{\text{age}^{-0.203} \cdot (0.742 \text{ for females})} \quad (10)$$

Serum protein levels

Prior to and following bariatric surgery induced weight loss, human serum albumin levels remained consistent with the

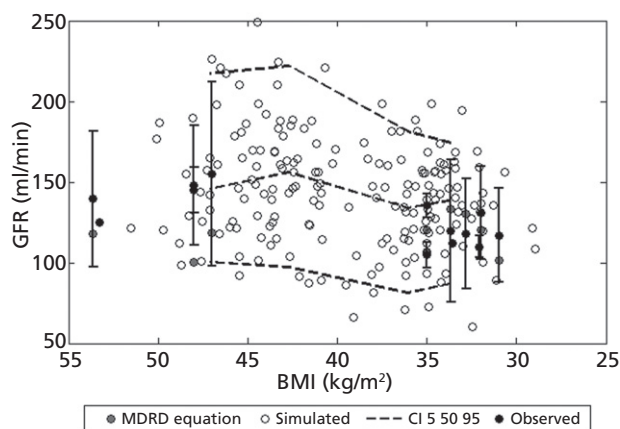


Figure 6 Observed glomerular filtration rate (GFR) following bariatric surgery induced weight loss as compared with calculated GFR utilising the modification of diet in renal disease (MDRD) equation and simulated age- and gender-matched GFR with 5, 50 95% confidence intervals (CI) utilising the Simcyp Simulator (MDRD) with inter-individual variability. BMI, body mass index.^[60–63]

normal reported range (at a total of 322 data points; $n = 163$) evaluated utilising sex- and age-matched simulations in the Simcyp Simulator, predicting human serum albumin within the 95% confidence interval (Figure 7).^[65–68] Levels of α -1 acid glycoprotein were significantly reduced following bariatric surgery induced weight loss (at a total of 170 data points; $n = 50$), regressing towards ranges observed in normal weight controls, where simulations in the Simcyp Simulator overestimated the levels of α -1 acid glycoprotein at lower BMI ranges (Figure 8).^[65,69]

Hepatic function

The reduction in liver volume following bariatric surgery induced weight loss was assumed to be a function of the reduction in body surface area as observed in a general population,^[70] where the equation incorporated into the Simcyp Simulator corrects for the observed under-prediction in liver volume at a BMI ≥ 40 kg/m² utilising a correction factor of 1.25.^[33] Tissue blood perfusions were obtained as a function of cardiac output estimated from body surface area as incorporated into the Simcyp Simulator. A summary of altered physiological parameters are provided in Table 2.^[71]

Virtual studies

Roux-en-Y gastric bypass

Simulated simvastatin immediate release 10 mg oral drug exposure post RYGB (small intestinal transit time 3.0 h) displayed an unaltered oral bioavailability with a mean post/pre surgery AUC ratio of 1.14 ± 0.18 due to a mean increase in F_G from 0.24 ± 0.10 to 0.27 ± 0.11 counteracted by a reduction

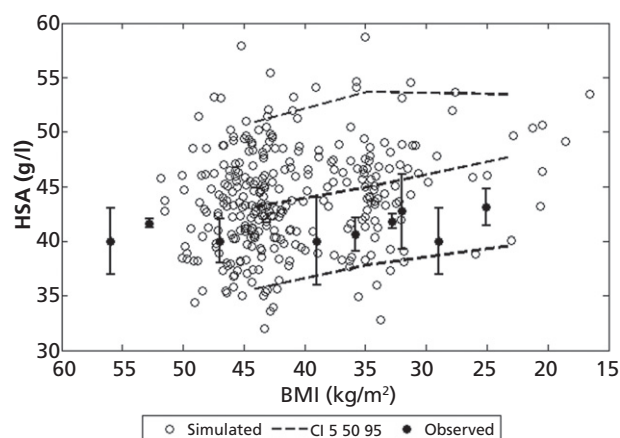


Figure 7 Observed serum concentrations human serum albumin (HSA) in morbidly obese patients subject to bariatric surgery induced weight loss as compared with simulated HSA levels with 5, 50 95% confidence intervals (CI) based on Simcyp demographics characteristics. BMI, body mass index.^[65–68]

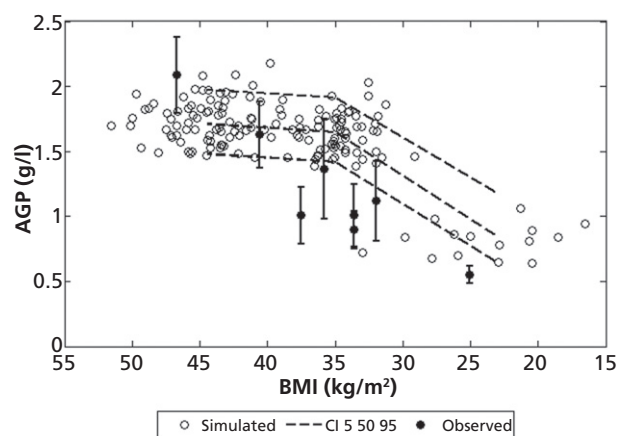


Figure 8 Observed serum concentrations (mean \pm SD) of α -1 acid glycoprotein (AGP) in morbidly obese patients subject to bariatric surgery induced weight loss as compared with simulated AGP levels with 5, 50 95% confidence intervals (CI) based on Simcyp Simulator demographics characteristics. BMI, body mass index.^[65,69]

in f_a from 0.90 ± 0.11 to 0.87 ± 0.12 (Figure 9). At a high therapeutic dose (80 mg) the mean post/pre surgery ratio became less apparent (1.07 ± 0.19) due to a more apparent reduction in f_a from 0.88 ± 0.12 to 0.82 ± 0.14 (Figure 10). Assuming a reduction in small intestinal motility post RYGB (small intestinal transit time 5.0 h) simvastatin displayed a mean ratio of 1.22 ± 0.19 to 1.17 ± 0.20 over the therapeutic dose range due to reduced postoperative impact on f_a . This was apparent over the whole range of studied drugs, where the increased small intestinal transit time positively influenced f_a (data not shown).

Oral drug exposure of omeprazole remained unaltered following RYGB (small intestinal transit time 3.0 h), although displaying a reduction in t_{max} from approximately 1.24 ± 0.41 to 0.97 ± 0.23 h over the therapeutic dose range. Diclofenac post/pre surgery AUC ratio displayed a minor reduction following RYGB (small intestinal transit time 3.0 h). This became more apparent at a high therapeutic dose, displaying an AUC ratio of 0.99 ± 0.14 , due to a reduction in f_a from 0.88 ± 0.13 to 0.84 ± 0.13 , counteracted by a minor increase in F_G from 0.95 ± 0.04 to 0.96 ± 0.03 ; whereas t_{max} displayed a reduction from 1.44 ± 0.54 to 1.28 ± 0.51 h. Ciprofloxacin displayed a minor reduction in AUC post RYGB (small intestinal transit time 3.0 h), displaying a ratio of 0.96 ± 0.02 over the therapeutic dose range due to a reduction in f_a from 0.77 ± 0.15 to 0.74 ± 0.15 . Fluconazole remained unaltered over the dose range.

Biliopancreatic diversion with duodenal switch

Following BPD-DS (small intestinal transit time 2.2 h), simvastatin displayed a reduction in AUC, with an observed post/pre surgical AUC ratio ranging from 0.89 ± 0.15 to

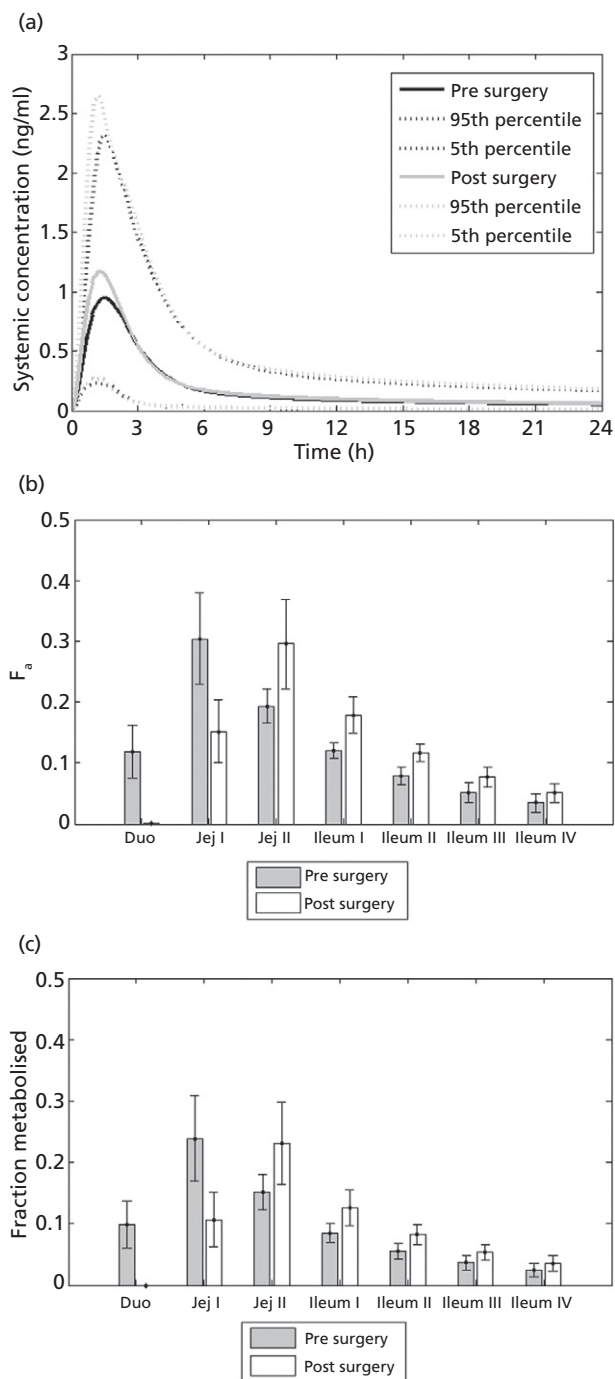


Figure 9 Simulated simvastatin immediate release 10 mg (low therapeutic dose) in morbidly obese ($n = 100$) and post Roux-en-Y gastric bypass surgery ($n = 100$; small intestinal transit = 3.0 h). (a) Mean, 95th and 5th percentile plasma concentration time profile over 24 h. (b) Mean \pm SD of segmental fraction of dose absorbed along the small intestine (f_a). (c) Mean \pm SD of segmental fraction of dose metabolised in the gut wall ($1 - F_G$). Duo, duodenum; Jej, jejunum.

Table 2 Summary of physiological parameter alterations following bariatric surgery for input into the Simcyp Simulator

Physiological parameters	RYGB	BPD-DS	JIB	SG	References
Population alterations					
Stomach					
Gastric emptying time (min)	7 (CV 45%)	Unaltered	Unaltered	13.6 (CV 53%)	[40,42]
Initial fluid volume (ml)	9.9 (CV 30%)	Unaltered	Unaltered	24.2 (CV 30%)	
Gastric pH	6.4 (CV 38%)	1.5 (CV 38%)	1.5 (CV 38%)	1.5 (CV 38%)	[38,39]
Small intestine					
Bypass (segments)	Duo, jej I ^b	Jej I, jej II	Jej II-IL III	Unaltered	[4,7,8,37,47–49,57–59]
Bile delay (segments)	Duo-jej II	Duo-il II		Unaltered	
SIT: scenario 1 (h)	3.0	2.2	0.4	3.3	
Weibull β^a	3.6	2.6	0.5	4.0	
SIT: scenario 2 (h)	5.0	3.7	0.7	–	
Weibull β^a	6.0	4.4	0.8	–	
GI metabolism					
CYP3A bypass (segments)	Duo, jej I ^b	Jej I, jej II	Jej II-IL III	Unaltered	[4,7,8,14,37,47–49,57–59]
CYP3A4 abundance (nmol/total gut)	50.2 (CV 60%)	30.0 (CV 60%)	32.3 (CV 60%)	66.2 (CV 60%)	
CYP3A5 abundance (nmol/total gut)	18.7 (CV 60%)	11.2 (CV 60%)	12.1 (CV 60%)	24.2 (CV 60%)	
Whole-body physiological alterations					
GFR prediction	MDRD	MDRD	MDRD	MDRD	[60–63]
Study design alterations					
Concomitant fluid intake with administered dose (ml)	30 (CV 60%)	150 (CV 60%)	250 (CV 60%)	80 (CV 60%)	[4,7,8,14,37,47–49,57–59]

BPD-DS, biliopancreatic diversion with duodenal switch; duo, duodenum; GFR, glomerular filtration rate; GI, gastrointestinal; IL, ileum; jej, jejunum; JIB, jejunoileal bypass; MDRD, modification of diet in renal disease equation; RYGB, Roux-en-Y gastric bypass; SG, sleeve gastrectomy; SIT, small intestinal transit. ^aWeibull distribution function ($\alpha = 2.92$; Equation 9). ^bPartial small intestinal bypass.

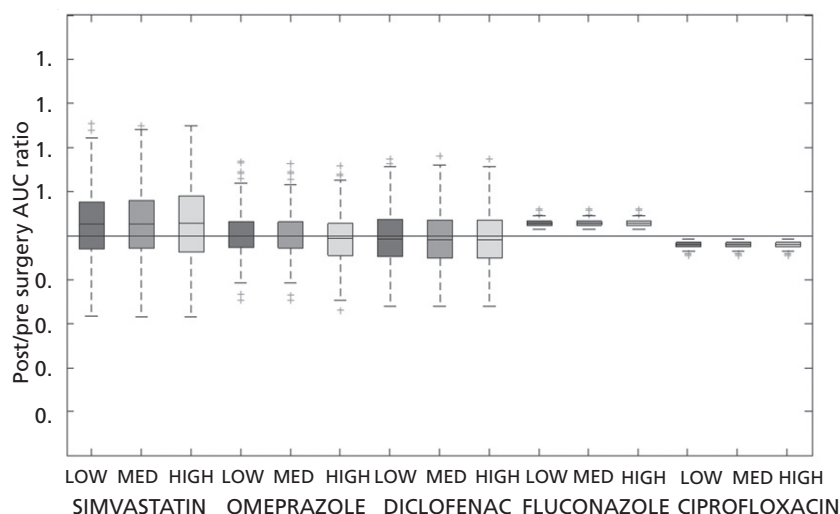


Figure 10 Simulated post/pre Roux-en-Y gastric bypass surgery (small intestinal transit = 3.0 h) AUC ratio over a range of selected drugs at a low, medium (MED) and high therapeutic dose: simvastatin immediate release (10, 20 and 80 mg), omeprazole enteric coated (10, 20 and 40 mg), diclofenac enteric coated (25, 50 and 75 mg), fluconazole immediate release (50, 200, 400 mg) and ciprofloxacin immediate release (250, 500 and 750 mg).

0.65 ± 0.22 as a result of a more extensive reduction in f_a as compared with following RYGB; assuming a higher small intestinal transit time of 3.7 h, simvastatin displayed an increase in AUC, displaying a ratio of 1.05 ± 0.08 at a low therapeutic dose level ranging to a reduction with a simulated ratio of 0.83 ± 0.22 at the highest therapeutic dose. This was observed for the whole range of simulated drugs.

Omeprazole displayed a post/pre BPD-DS AUC ratio of 0.88 ± 0.10 at a low therapeutic dose due to a reduction in f_a from 0.94 ± 0.09 to 0.83 ± 0.14 (Figure 11), whereas a minor increase in F_G was observed from 0.96 ± 0.02 to 0.97 ± 0.02 . T_{max} displayed an increase from 1.22 ± 0.38 to 1.50 ± 0.54 h, whereas C_{max} displayed a reduction by approximately 19%. At a high therapeutic dose, omeprazole

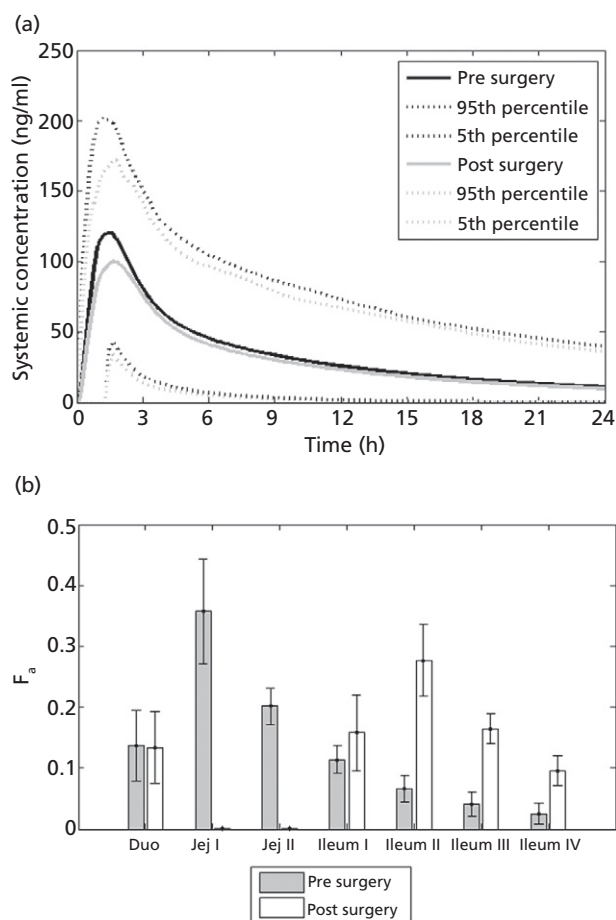


Figure 11 Simulated omeprazole enteric coated 10 mg (low therapeutic dose) in morbidly obese ($n = 100$) and post biliopancreatic diversion with duodenal switch ($n = 100$; small intestinal transit = 2.2 h). (a) Mean, 95th and 5th percentile plasma concentration time profile over 24 h. (b) Mean \pm SD of segmental fraction of dose absorbed along the small intestine (f_a). Duo, duodenum; Jej, jejunum.

displayed a post/pre surgery AUC ratio of 0.77 ± 0.15 , due to a more extensive reduction in f_a , whereas t_{max} was increased from 1.42 ± 0.50 to 2.26 ± 0.63 h. The reduction became less apparent assuming a small intestinal transit time of 3.7 h.

Diclofenac displayed an AUC ratio of 0.87 ± 0.09 following BPD-DS (small intestinal transit time 2.2 h) at a low therapeutic dose due to a reduction in f_a from 0.89 ± 0.12 to 0.75 ± 0.15 , whereas F_G displayed an increase from 0.91 ± 0.06 to 0.94 ± 0.04 . At a high therapeutic dose, diclofenac displayed a more apparent reduction due to a higher post surgical impact on f_a . Again the reduction was less apparent assuming a small intestinal transit time of 3.7 h.

Fluconazole displayed an AUC ratio of approximately 0.95 ± 0.05 over the dose range. Ciprofloxacin displayed an AUC ratio of 0.80 ± 0.06 following BPD-DS (small intestinal transit time 2.2 h) at a low therapeutic dose, reflected by a

reduction in f_a . Following BPD-DS (small intestinal transit time 3.7 h), Ciprofloxacin displayed no significant alteration, with an AUC ratio of 1.01 ± 0.01 at a low therapeutic dose ranging to 0.98 ± 0.01 at a high therapeutic dose (Figure 12).

Jejunioleal bypass

Following jejunioleal bypass the whole range of studied drugs displayed an extensive reduction in AUC due to a more apparent reduction in f_a as compared with RYGB and BPD-DS where fluconazole displayed the least apparent reduction, with a post/pre surgery AUC ratio of 0.47 ± 0.12 at a low therapeutic dose, whereas an AUC ratio of 0.44 ± 0.13 was displayed at a high dose level due to a more extensive reduction in f_a from 0.97 ± 0.07 to 0.45 ± 0.13 (Figures 13 and 14).

Sleeve gastrectomy

Simulated post sleeve gastrectomy applied to the 'morbidly obese' population did not significantly alter the pre to post surgery drug exposure for the range of studied drugs over low to high therapeutic dose ranges (data not shown).

Discussion

Simulating oral drug exposure following bariatric surgery

Simulating oral drug bioavailability following bariatric surgery identified a number of potential pharmacokinetic parameters suggested to influence bioavailability following bariatric surgery.

Simvastatin is characterised as a BCS class IV drug, and further classified as a Biopharmaceutics Drug Disposition Classification System (BDDCS) class II compound.^[26,72] The drug is considered a low soluble compound at the therapeutic dose, displaying an aqueous solubility 0.03 mg/ml.^[73,74] The drug is administered in its lactone form and undergoes pH- and temperature-dependent interconversion to its hydroxyacid form at a pH below 6, whereas the lactone form is mainly formed at pH values over the equilibrium.^[75] Approximately 85% of the administered dose is absorbed, being further exposed to extensive metabolism by CYP3A4 in the small intestine and liver, and CYP3A5 to lesser extent.^[76,77]

The simulated increase in drug exposure of simvastatin in the post RYGB (small intestinal transit time 3.0 h) population was due to an increase in F_G post surgery. These findings suggest intestinal gut wall metabolism plays an important role in the observed trend in drug bioavailability pre to post surgery for compounds subject to a high small intestinal metabolic extraction ratio, such as atorvastatin and simvastatin, where the simulated post/pre surgical AUC ratio following RYGB was similar to that observed for atorvastatin, displaying a median AUC ratio of 1.20 (0.3–2.3).^[49] Simulated

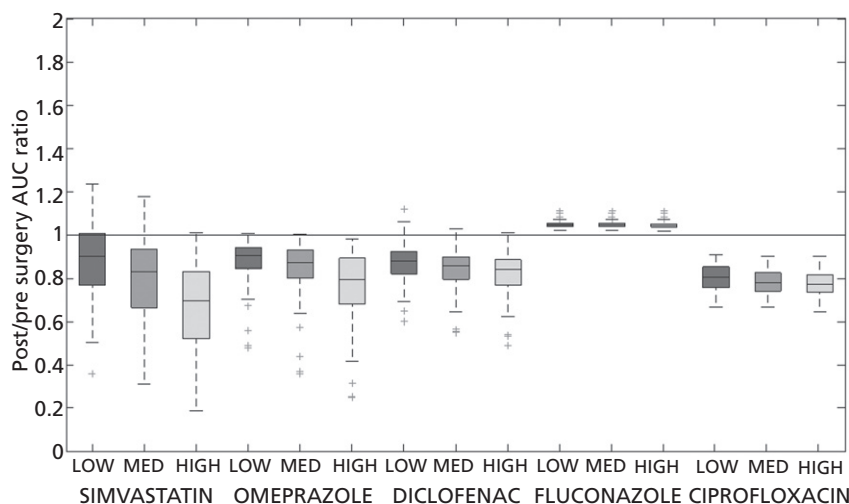


Figure 12 Simulated post/pre biliopancreatic diversion with duodenal switch (small intestinal transit = 2.2 h) AUC ratio over a range of selected drugs at a low, medium (MED) and high therapeutic dose: simvastatin immediate release (10, 20 and 80 mg), omeprazole enteric coated (10, 20 and 40 mg), diclofenac enteric coated (25, 50 75 mg), fluconazole immediate release (50, 200, 400 mg) and ciprofloxacin immediate release (250, 500 and 750 mg).

compound characteristics of simvastatin did not incorporate the pH-dependent interconversion of the lactone and acid form,^[75] but treated this as a part of the CYP3A4 clearance term through fitting to observed data, thus not taking into account the increased gastric pH following RYGB surgery and its impact on the interconversion.

Omeprazole (BCS class II and BDDCS class I ampholyte, $pK_a = 8.7$, $pK_b = 3.79$) is a sparingly soluble highly lipophilic compound with stability issues at a lower pH levels, thus motivating the enteric coated formulation to protect the drug from degradation caused by the gastric pH.^[26,72,78,79] The drug displays a highly variable absorption and further mainly undergoes hepatic metabolism and clearance by CYP3A4 and 2C19.^[80] Only a minor alteration in F_G was observed following simulations post BPD-DS, where an overall increase was observed. The biggest impact was observed on f_a , potentially due to the reduction in absorption area.

Diclofenac (BCS class II, BDDCS class I) is mainly metabolised by CYP2C9.^[26,71,79] The drug undergoes extensive first-pass metabolism, displaying an oral bioavailability of approximately 54%.^[80,81] Following RYGB and BPD-DS, a minor increase in F_G was observed due to the bypass of intestinal regions abundance of CYP2C9, however this was counteracted by a reduction in f_a .

Fluconazole (BCS class I, BDDCS class III) is soluble at the therapeutic dose and displays a bioavailability of over 90% in healthy volunteers, and further is mainly renally cleared.^[26,72,82] Following bariatric surgery simulated oral drug exposure of fluconazole only displayed minor changes in AUC, with the exception following jejunoileal bypass. These results are consistent with observations in AIDS patients, frequently displaying gastrointestinal disturbances,

and a case report in a patient subject to gastrointestinal restriction of the gastric antrum, duodenum and ileum following peptic ulcer disease, displaying no altered bioavailability or a comparable bioavailability as compared with healthy volunteers.^[83,84]

Ciprofloxacin (BCS class III, BDDCS class IV) is sparingly soluble at the therapeutic dose range, further having a reported oral bioavailability ranging from approximately 60% to 80% in healthy volunteers, and is mainly renally cleared.^[26,72,85,86] The simulated reduction in AUC following bariatric surgery is therefore most likely an effect of a reduction in absorption area and a product of postoperative solubility issues.

The major issue following sleeve gastrectomy would be potential solubility issues due to a reduced concomitant fluid volume with the administered dose, although this was not a major issue for any of the studied drugs.

Post bariatric surgery ADAM model limitations

Conclusions drawn from this study are limited by a number of 'known unknowns' relating to gastrointestinal physiology post bariatric surgery, where data relating to gastrointestinal pH, small intestinal transit and post surgical gastrointestinal physiological adaptation and whole-body physiological alterations, such as hepatic activity and bile secretion and its GI levels, is sparse or nonexistent.

Following RYGB, gastric pH was estimated to increase based on measuring acid secretion in the gastric pouch (mEq/time). However, examining the relationship between pH and gastric acid output is not straightforward. Pratha

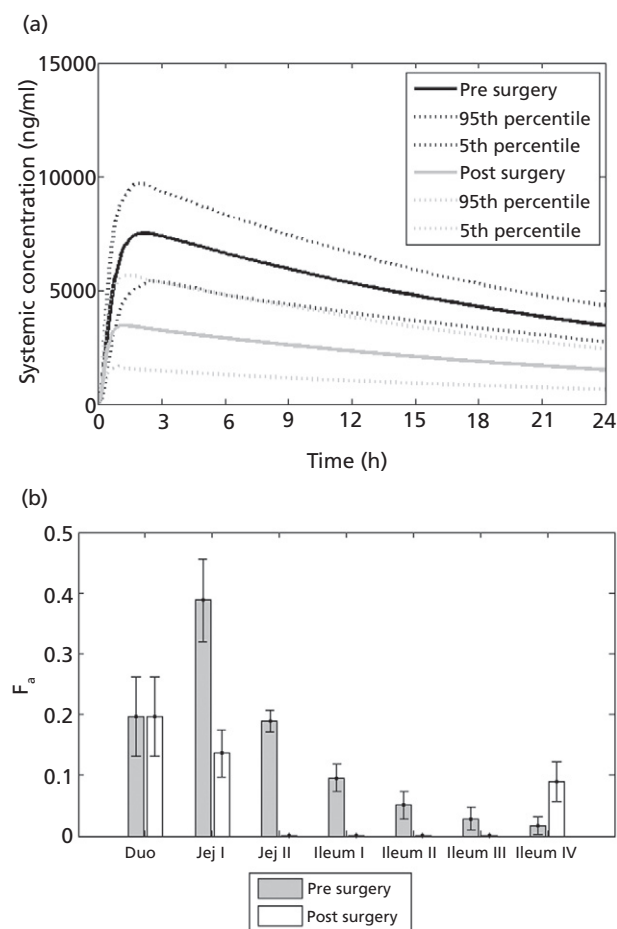


Figure 13 Simulated fluconazole immediate release 400 mg (high therapeutic dose) in morbidly obese ($n = 100$) and post jejunoileal bypass ($n = 100$; small intestinal transit = 0.4 h). (a) Mean, 95th and 5th percentile plasma concentration time profile over 24 h. (b) Mean \pm SD of segmental fraction of dose absorbed along the small intestine (f_a). Duo, duodenum; Jej, jejunum.

et al.^[87] examined the effect of proton pump inhibitors on gastric acid output and pH and concluded the relationship between pH and gastric acid output to be highly ambiguous. At a gastric acid output of ≤ 1 mEq/30 min a pH of 0.9–7.7 was observed, whereas a pH of 2.5 and upwards was rendered at minimal gastric acid output,^[87] thus rendering a high degree of uncertainty in the implications of mEq/time post RYGB.

Small intestinal transit time estimation following bariatric surgery was limited to one study examining small intestinal transit time of solids in 10 patients subject to total gastrectomy with Roux-en-Y reconstruction^[50] or estimations based on the extent of small intestinal bypass. As the procedure differs in terms of the extent of gastrectomy as compared with RYGB for the treatment of obesity, such an assumption may not necessarily hold true.

Following gastric restrictive surgery (RYGB and sleeve gastrectomy), gastric emptying of liquid displayed an overall significant reduction, whereas gastric emptying of solids displayed an increase in variability following RYGB. The impact of RYGB surgery on gastric emptying of solids may be due to a postsurgical state of stasis due to a reduced nervous stimulus.^[42,54]

The methodology of how the ADAM model was adapted to mimic post bariatric surgery conditions is subject to a number of limitations due to the limited nature of how the ADAM model could be adjusted through the Simcyp Simulator through the existing interface. Rather than bypassing the proximal small intestinal compartments, the transit times through these compartments were reduced to close to zero. As a consequence the modelling and simulations of drug concentration in the biliary limb could not be conducted, thus limiting the predictability of drugs subject to biliary elimination. A further concern was the fluid dynamics within the ADAM model which is governed by secretion and reabsorption of GI fluids taking place throughout the GI compartments.^[14,35] As a result of such parameter alterations not being possible through the Simcyp user interface, an overestimation of GI fluid volumes and consequential underestimation of potential drug specific solubility issues following surgery are possible.

Conclusions

Trends in pre and post RYGB bioavailability seem to be highly dependent on drug-specific parameters such as affinity to CYP3A4, solubility and permeability issues based on simulated outcomes, although this has yet to be confirmed with regards to clinical data. A mechanistic modelling approach has the potential of examining the impact of drug-specific parameters on trends pre to post surgery and to serve as a useful tool in examining the impact of physiological alterations on oral drug bioavailability in the absence of clinical data.

Current limitations in estimating and simulating the impact of oral drug bioavailability following bariatric surgery include the sparsity of clinical data for further model validation and the lack of data on resultant physiological changes post surgery.

Declarations

Conflict of interest

Amin Rostami, Devendra Pade and Masoud Jamei are employees and/or shareholders in Simcyp Limited.

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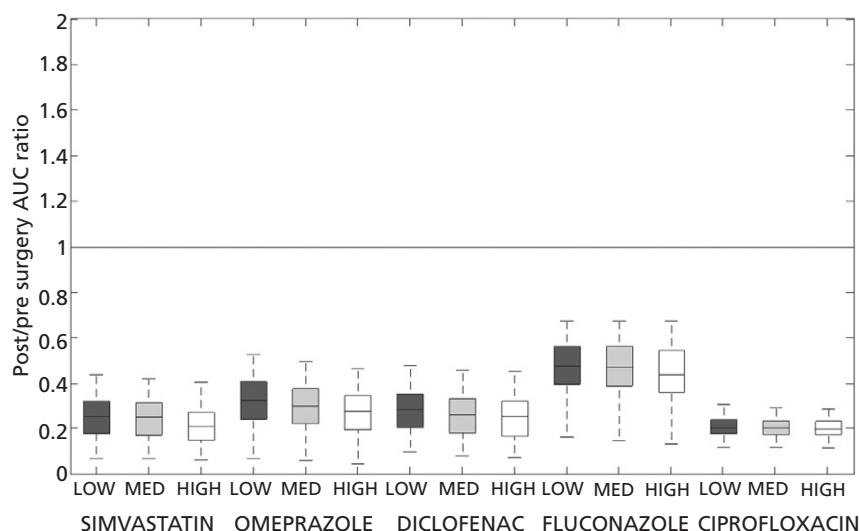


Figure 14 Simulated post/pre jejunoileal bypass (small intestinal transit = 0.4 h) AUC ratio over a range of selected drugs at a low, medium (MED) and high therapeutic dose: simvastatin immediate release (10, 20 and 80 mg), omeprazole enteric coated (10, 20 and 40 mg), diclofenac enteric coated (25, 50 75 mg), fluconazole immediate release (50, 200, 400 mg) and ciprofloxacin immediate release (250, 500 and 750 mg).

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8.2.2 Compound Simcyp Simulator template input properties

Table 8.3. Drug specific parameters as incorporated into Simcyp® Simulator.

Parameters	CPF	DCF	Drugs FCZ	OMZ	SIM
PhysChem					
MW (g/mol)	331.4	296.2	306.3	345.4	418.6
LogP _{o:w}	0.3	4.5	0.2	2.23	4.68
Acid-base nature	Ampholyte	Acid	Base	Ampholyte	Neutral
pKa	5.88	4.01	1.76	8.7	NA
pKb	8.74			4.4	
Blood binding					
BP	0.75	0.61	1	0.59	1
f _{u,p}	0.79	0.003	0.89	0.043	0.011
Dissolution					
Formulation	IR	EC	IR	EC	IR
Solubility input	Predicted	Predicted	Predicted	Predicted	Predicted
S ₀ (mg/mL)	26.324	0.001	30.630	0.322	0.001
Absorption					
IVIVC method	PSA	PSA	Caco-2, pH6.5:7.4 P _{app} : 29.8·10 ⁻⁶ cm/s	MDCK: P _{app} : 59·10 ⁻⁶ cm/s	PSA
	PSA: 72.9 HBD: 2	PSA: 49.3 HBD: 2			PSA: 72.83 HBD: 1
P _{eff,man} (10 ⁻⁴ cm/s)	1.25	2.27	4.27	3.25	2.37
Distribution					
Model	1-comp.	1-comp.	1-comp.	1-comp.	1-comp.
Estimation method	V _{ss,iv}	V _{ss,iv}	V _{ss,iv}	V _{ss,iv}	V _{ss,iv}
V _{ss} (L/kg)	2.48	0.195	0.748	0.35	2.13
Elimination					
Metabolism	NA	CYP2C9 V _{max} : 8.28 ^A K _{m,u} : 0.71 ^B	CL _{iv} : 1.01 L/h	CYP2C19 V _{max} : 6.47 ^A K _{m,u} : 1.28 ^B	CYP3A4 CL _{int} : 2597 ^D
		UGT2B7 V _{max} : 2800 ^C K _{m,u} : 2.45 ^B		CYP3A4 V _{max} : 2.3 ^A K _{m,u} : 58.5 ^B	
				CYP3A4 V _{max} : 12.2 ^A K _{m,u} : 137 ^B	
CL _R (L/h)	23.7	1.05	0.7	0.037	NA

References: (Turner, 2008)

CPF=Ciprofloxacin, DCF=Diclofenac, FCZ=Fluconazole, OMZ=Omeprazole, SIM=Simvastatin, MW=Molecular weight, LogP_{o:w}=Octanol:Water partitioning coefficient, BP=Blood to plasma ratio, f_{u,p}=fraction unbound in plasma, S₀=intrinsic aqueous solubility, IVIVC=*In vitro-in vivo* correlation, P_{eff,man}=Estimated human permeability, CYP=Cytochrome P450, CL_R=Typical renal clearance in healthy volunteers, V_{ss}=Volume of distribution at steady state, iv=Intravenous infusion, NA=Not applicable.

^A pmol/min/mg microsomal protein

^B μM

^C pmol/min/mg protein

^D μL/min/mg microsomal protein

8.3 Evaluation of an *in silico* PBPK post-bariatric surgery model through simulating oral drug bioavailability of atorvastatin and cyclosporine

8.3.1 Publication in Clinical Pharmacology and Therapeutics:

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ORIGINAL ARTICLE

Evaluation of an *In Silico* PBPK Post-Bariatric Surgery Model through Simulating Oral Drug Bioavailability of Atorvastatin and Cyclosporine

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An increasing prevalence of morbid obesity has led to dramatic increases in the number of bariatric surgeries performed. Altered gastrointestinal physiology following surgery can be associated with modified oral drug bioavailability (F_{oral}). In the absence of clinical data, an indication of changes to F_{oral} via systems pharmacology models would be of value in adjusting dose levels after surgery. A previously developed virtual “post-bariatric surgery” population was evaluated through mimicking clinical investigations on cyclosporine and atorvastatin after bariatric surgery. Cyclosporine simulations displayed a reduced fraction absorbed through gut wall (f_a) and F_{oral} after surgery, consistent with reported observations. Simulated atorvastatin F_{oral} postsurgery was broadly reflective of observed data with indications of counteracting interplay between reduced f_a and an increased fraction escaping gut wall metabolism (F_g). Inability to fully recover observed atorvastatin exposure after biliopancreatic diversion with duodenal switch highlights the current gap regarding the knowledge of associated biological changes.

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The prevalence of obesity has increased dramatically in the USA and Europe over the past decade.^{1,2} Bariatric surgery has proven to be successful in treating morbid obesity with over 220,000 surgeries performed in the USA and Canada in 2008.³ Several bariatric surgical methods coexist in healthcare, where Roux-en-Y gastric bypass (RYGB) is considered the gold standard.⁴ RYGB results in a reduced gastric volume, complete bypass of the pylorus, partial bypass of the duodenum and proximal jejunum, and a delay in bile inflow to the distal jejunum. The more invasive biliopancreatic diversion with duodenal switch (BPD-DS) results in a partial resection of the stomach with the pylorus retained, bypass of jejunum and proximal ileum, and an approximately 250 cm delay of the bile inlet. Jejunoleal bypass (JIB) is considered to be the most invasive procedure, retaining only the stomach (with pylorus) and distal ileum.^{5,6}

As a consequence of bariatric surgery, a number of physiological parameters influencing oral drug bioavailability (F_{oral}) are altered, including: a reduced gastric capacity and emptying time, altered gastrointestinal (GI) pH, reduced absorption area, altered bile flow and small intestinal transit (SIT), altered substrate exposure to drug-metabolizing enzymes, and active efflux transporters.^{5,7,8} Patients undergoing bariatric surgery continue to receive various therapeutic drugs without dose adjustments for altered bioavailability, which can potentially lead to no therapeutic effect or higher than required systemic exposure. There are a very limited number of studies that have investigated oral drug exposure post-bariatric surgery.^{5,9}

The direction and magnitude of impact on F_{oral} following surgery may depend on the characteristics and invasiveness

of the surgical procedure,^{10,11} where the extent of the small intestinal bypass may influence the fraction of dose absorbed through the gut wall (f_a). Bypassing regions highly abundant in drug-metabolizing enzymes can affect the fraction of absorbed drug F_g .⁶ F_H , the fraction that escapes hepatic first-pass metabolism, may be assumed to remain unaltered (Eq. 1).^{5,7,8}

$$F_{\text{oral}} = f_a \cdot F_g \cdot F_H \quad (1)$$

A level of uncertainty remains regarding the SIT postsurgery, where a reduction in motility has been observed, albeit well-powered clinical studies of SIT in man are lacking.^{6,12,13}

The postsurgical physiology is further complicated by the possibility of small intestinal trauma or adaptation, where an enhanced permeability due to impairment of the mucosa or long-term villi elongation has been observed in rat BPD-DS models.^{14,15} Alterations in the levels of gastric hormones (including: peptide YY, ghrelin, and Glucagon-Like Peptide 1) may lead to redistribution of intestinal blood flow to the submucosa, as observed in dog models. Postsurgical hormonal levels have been observed to vary depending on the bariatric surgical procedure.^{13,16–18}

Due to these multifactorial changes, physiologically based pharmacokinetic (PBPK) modeling enables one to predict, *in silico*, the effects of various bariatric surgeries in a morbidly obese population.⁶ The Advanced Dissolution Absorption and Metabolism (ADAM) model describes the variability in F_{oral} through a physiologically based seven-segment model of the small intestine, including: duodenum, jejunum I and II, and ileum I–IV. The model describes drug release from formulation, dissolution, precipitation,

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degradation, absorption, active transport, and metabolism as the drug transits through the small intestine, allowing the incorporation of saturation effects and population variability. The ADAM model has been well described and used in the previous literature.^{8,19}

In our previous work, a virtual “post-bariatric surgery” population was created using the ADAM model within a PBPK system containing characteristics of a morbidly obese population. Developed models for RYGB, BPD-DS, and JIB included specific anatomical and physiological parameters that are altered following surgery, namely: gastric capacity and fluid dynamics, gastric emptying time, small intestinal bypass, GI pH, bile flow, and alterations to regional abundance of drug-metabolizing enzymes (e.g. CYP3A) and efflux transporter P-glycoprotein. The model further incorporated whole body physiological changes, such as postsurgical recovery of renal function as a function of weight loss.⁶

Simulations predicted change in oral bioavailability of various drugs pre- to post-bariatric surgery, revealing the magnitude and direction of the effect to be surgery dependent, due to altered GI system parameters, and influenced by a complex interplay between drug characteristics, including: solubility, permeability, dissolution, gut wall metabolism, and dose level. However, no comparison so far has been made between the results of these simulations and existing clinical data.⁶ In the current study, we report on the evaluation of

previously developed post-bariatric surgery models by comparing the observed vs. predicted impact of bariatric surgery on oral exposure of cyclosporine and atorvastatin acid using virtual simulations.

RESULTS

Changes in oral drug bioavailability after bariatric surgery were demonstrated for cyclosporine and atorvastatin acid following RYGB, BPD-DS, and JIB.^{10,11,20,21} Sex-, age-, height-, and weight-matched simulations were carried out based on the corresponding clinical studies using post-bariatric surgery models coupled to a full PBPK distribution model into the Simcyp Simulator (Simcyp Limited (a Certara Company), Sheffield, UK). The results from the comparison of observed vs. simulation studies are as follows:

Cyclosporine

Roux-en-Y gastric bypass. Following RYGB, Marterre and coworkers reported a 194% increase in the daily dose per kg body weight in kidney transplant patients ($n = 3$) of cyclosporin A (CsA) Sandimmune solution. CsA trough blood levels were monitored from 6 months before RYGB up to 12 months postoperatively, using an immunoassay technique (TDx, Abbott Laboratories). The observed reduction in exposure prompted an increase in the oral dose from 1.8 (± 0.5) to 3.5

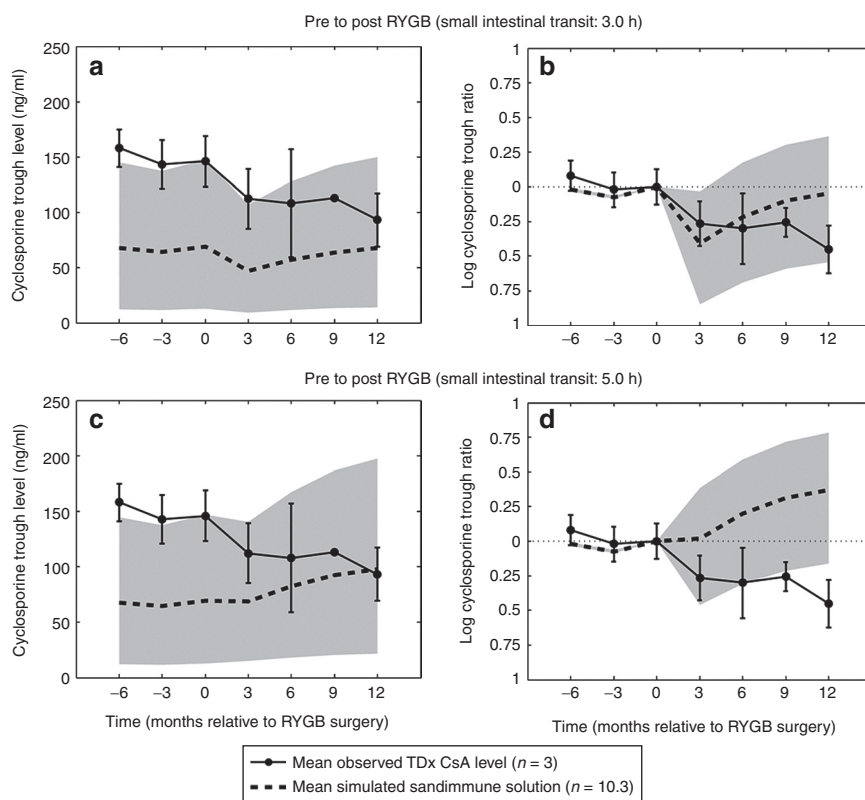


Figure 1 Mean and SD of observed cyclosporin A (CsA) TDx trough levels at steady state pre to post-Roux-en-Y gastric bypass (RYGB) at -6, -3, 0, 3, 6, 9, and 12 months relative to RYGB surgical event (0 months). Time points from -6 to 12 months correspond to dose levels of 1.7, 1.7, 1.8, 2.4, 2.8, 3.2, 3.5 mg/kg/day, respectively ($n = 3$) administered twice daily. Observed data are compared with simulated 50, 95, and 5% prediction interval, indicated by gray area, of CsA Sandimmune trough levels ($n = 10 \times 3$). (a) Simulated post-RYGB at a small intestinal transit time (SIT) of 3.0h, (b) log-normalized simulated CsA trough ratio as compared with 0 months (RYGB SIT = 3.0h), (c) simulated CsA trough levels at RYGB SIT of 5.0h, (d) log-normalized simulated CsA trough ratio as compared with 0 months (RYGB SIT = 5.0h).²⁰

(± 1.1) mg/kg/day in order to maintain pre-RYGB CsA trough levels (20) (**Figure 1a–d**). Owing to the reported overprediction of the TDx immunoassay, observed and simulated data were normalized for trough levels immediately before RYGB surgery, indicated by the time of 0 months (**Figure 1b,c**).²²

In an age-, sex-, and weight-matched virtual population, oral drug exposure of Sandimmune CsA solution was simulated in 10 randomized trials consisting of 3 individuals in each trial ($n = 10 \times 3$). Cyclosporine displayed a reduction in f_a from 0.40 (5–95% confidence interval (CI95): 0.24–0.59) to 0.19 (0.10–0.32) following RYGB, at a simulated SIT time of 3.0 h, whereas F_g remained unaltered at 0.86 (0.74–0.87). A 194% increase in dose level, resulted in a trough level ratio of 0.96 (0.58–1.44) as compared with the preoperative exposure at 0 months. Assuming a postsurgical SIT time of 5.0 h, cyclosporine displayed reduction in f_a to 0.26 (0.14–0.41), and F_g remained unaltered. A 194% increase in the dose level resulted in an overprediction in post-RYGB CsA trough levels, with a simulated post/presurgical ratio of 1.45 (0.85–2.19) as compared with preoperative exposure at 0 months (**Figure 1a–d**).

Simulations of the theoretical impact of RYGB on the solubilization enhanced cyclosporine Neoral microemulsion, at a postsurgical SIT of 3.0 h, produced an area under the concentration–time curve (AUC) ratio of 1.84 (1.26–2.37) at 12 months postsurgery as compared with the levels at 0 months relative to RYGB surgery. The observed increase in oral exposure of Neoral was due to a 194% dose increase, where f_a displayed an increase from 0.72 (0.47–0.92) to 0.82 (0.57–0.94), whereas F_g increased from 0.90 (0.81–0.96) to 0.94 (0.90–0.98) (**Supplementary Data** online).

Jejunioleal bypass. In a case study by Chenhsu *et al.*,²¹ CsA blood levels at 2 h after administration at steady state (C₂), administered as Neoral microemulsion in controls ($n = 7$) and post-JIB ($n = 1$), displayed a reduced exposure when comparing the mean C₂ concentration over the administered dose range, reporting a reduction in C₂ levels of ~59%.

Simulating demographically matched morbidly obese controls ($n = 10 \times 7$) and post-JIB patients (SIT = 0.4 h; $n = 10 \times 1$), cyclosporine displayed a reduction in C₂ levels from 452 (153–776) to 357 (103–650) ng/ml at a dose level of 4 mg/kg/day and from 2,528 (388–6089) to 1,632 (571–2,811) ng/ml at a dose of 12 mg/kg/day. Simulated levels corresponded well with the linear regression of observed data as compared with the 5–95% prediction interval. The simulated reduction in oral drug exposure in the post-JIB population as compared with the controls was due to a reduction in f_a from 0.61 (0.35–0.86) to 0.12 (0.04–0.19), whereas F_g displayed a minor reduction from 0.90 (0.79–0.97) to 0.88 (0.75–0.96) at a therapeutic dose of 2 mg/kg/day. At a dose of 12 mg/kg/day, a major reduction in f_a was observed from 0.34 (0.16–0.53) to 0.08 (0.01–0.18), whereas F_g was reduced from 0.91 (0.81–0.93) to 0.90 (0.80–0.97) (**Figure 2**).

Assuming a SIT of 0.7 h after JIB, cyclosporine displayed a less apparent reduction in C₂ levels due to a less apparent reduction in f_a to 0.19 (0.05–0.30) and 0.13 (0.02–0.26) at corresponding dose levels of 2 and 12 mg/kg/day, respectively. After JIB (SIT = 0.7 h), F_g was altered to 0.89

(0.79–0.96) and 0.92 (0.84–0.98) at a therapeutic dose level of 2 and 12 mg/kg/day, respectively (**Supplementary Data** online).

Atorvastatin

Roux-en-Y gastric bypass. In a clinical trial carried out on 12 morbidly obese patients, atorvastatin was administered as an immediate release tablet of 20–80 mg in fasted state where patients were allowed to eat 2 h after administration. Plasma concentration profiles were obtained from 0–8 h after drug administration before and 3–6 weeks after RYGB. The pre to postsurgical trend in oral exposure displayed a high variability where the overall reported trend displayed a median post/pre surgery AUC ratio of 1.12 (range: 0.34–2.33), albeit being statistically insignificant.¹⁰

Virtual simulations for oral drug exposure of atorvastatin acid pre- to post-RYGB were conducted in 10 randomized trials, each consisting of 12 age-, sex-, and BMI-matched individuals ($n = 10 \times 12$). Assuming a reduction in SIT as function of the small intestinal bypass (SIT = 3.0 h) resulted in an overall increase in AUC with a simulated median post/presurgical AUC ratio of 1.13, capturing 100% of observed data within the simulated 95% prediction interval of 0.27–3.80 (**Figure 3a–j**). Alternatively, with an increase in SIT time post-RYGB (SIT = 5.0 h), atorvastatin acid displayed a median post/presurgical AUC ratio of 1.42 (0.34–4.91) (**Supplementary Data** online).

Simulated increase in exposure of atorvastatin following RYGB (SIT = 3.0 h) was due to a reduction in f_a from 0.58 (0.33–0.77) to 0.54 (0.29–0.74) counteracted by an increase in F_g from 0.69 (0.48–0.86) to 0.73 (0.53–0.88) (**Figure 4a,b**).

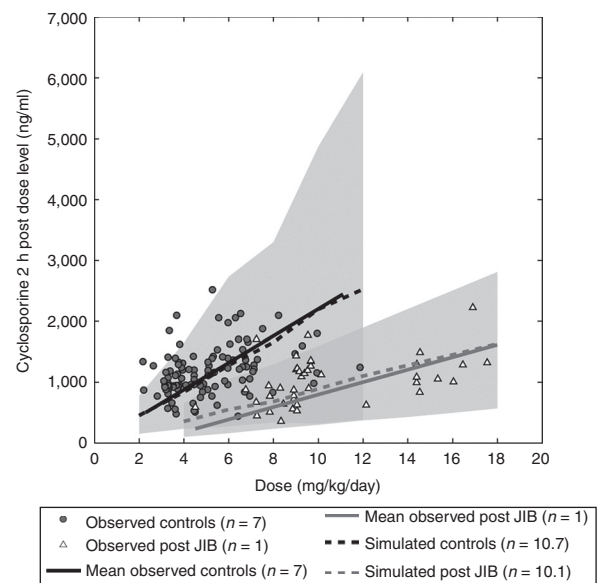


Figure 2 Observed mean blood concentration of cyclosporine microemulsion (Sandimmune Neoral; Novartis) at steady state 2 h postdosing in controls ($n = 10 \times 7$) and one patient ($n = 10 \times 1$) post-jejunoileal bypass (JIB) as compared with simulated sex- and age-matched controls ($n = 300$) and post-JIB ($n = 800$) at a small intestinal transit time of 0.4 h over dose range of 300–1,000 mg, where 5, 50, and 95% prediction intervals are indicated by gray areas.²¹

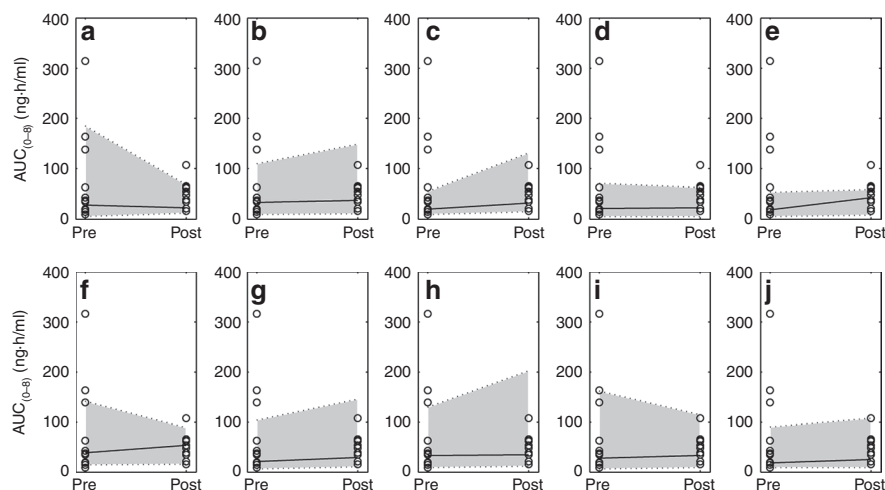


Figure 3 Simulated 50, 95, and 5% prediction interval (indicated by gray areas) of oral drug exposure of atorvastatin acid in randomized trials of age-, sex-, dose-, and BMI-matched patients pre- to post-Roux-en-Y gastric bypass surgery (small intestinal transit = 3.0 h) as compared with observed data. (a–j) Ten randomized simulated trials consisting of 12 individuals in each trial ($n = 10 \times 12$), as compared with observed ($n = 12$; open circles).¹⁰ AUC, area under the concentration–time curve.

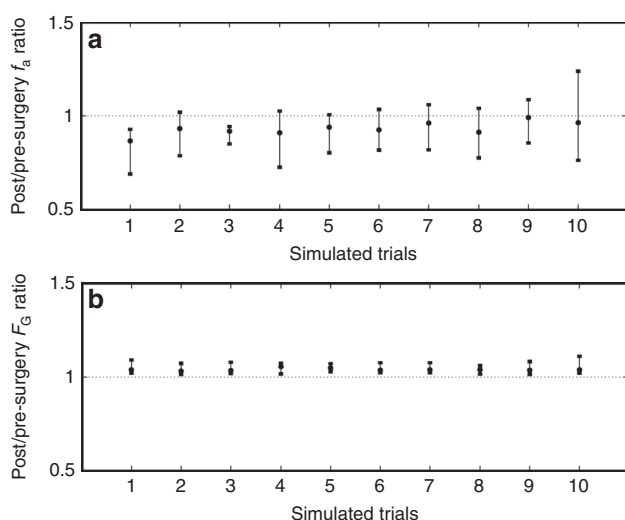


Figure 4 Simulated 50, 95, and 5% prediction intervals of the ratio of (a) fraction of dose absorbed in the intestine (f_a), and (b) fraction escaping gut wall metabolism (F_g) of atorvastatin acid pre- to post-Roux-en-Y gastric bypass surgery (small intestinal transit = 3.0 h) in 10 individually simulated randomized trials (1–10) consisting of 10 individuals in each pre- and postsurgery ($n = 10 \times 10$).

Assuming a reduced small intestinal motility (RYGB SIT = 5.0 h), the more apparent increase in AUC was the result of an extensive increase in f_a .

Biliopancreatic diversion with duodenal switch. Atorvastatin immediate release tablet 20–80 mg administered in the fasted state, allowing feeding at 2 h, displayed a significant increase in oral drug exposure following BPD-DS in 10 morbidly obese patients, with an observed mean AUC ratio of $2.0 (\pm 1.0)$ and observed increase in the C_{max} from 20.0 ng/ml (± 24.9) to 28.0 (± 22.5), whereas t_{max} increased from 1.2 h (± 0.8) to 2.3 h (± 1.0) post-BPD-DS.¹¹

Predicted plasma concentration–time profiles of atorvastatin acid were consistent with observed data before surgery in a morbidly obese population (**Supplementary Data** online).

However, simulated plasma concentration–time profiles following BPD-DS (SIT = 1.2 h) were unable to capture the observed increase in oral drug exposure. The predicted AUC ratio of 0.90 (0.16–2.24) was lower than expected due to a reduction in f_a from 0.61 (0.34–0.79) to 0.39 (0.06–0.72), which was counteracted by an increase in F_g from 0.69 (0.59–0.79) to 0.72 (0.63–0.81). C_{max} displayed a minor increase, with a post/pre-BPD-DS C_{max} ratio of 1.32 (0.31–2.38), whereas t_{max} displayed a post/pre-BPD-DS ratio of 0.62 (0.31–1.00). The simulated pre- to post-BPD-DS alterations in AUC, C_{max} , and t_{max} correspond to the central points of **Figure 5a–c**, respectively.

Sensitivity analysis was performed to assess the impact of potential physiological alterations postsurgery on the plasma exposure of atorvastatin acid, including the impact of: SIT, gastric emptying time, bile concentration in the terminal ileum, small intestinal enterocyte volume (V_{ent}), GI CYP3A content, and small intestinal permeability (P_{eff}). The AUC was insensitive to changes in the postsurgical bile concentration and V_{ent} . Following BPD-DS (SIT = 1.2 h), a fivefold increase in P_{eff} led to a post/presurgical AUC ratio of 1.93 (0.60–5.53), whereas C_{max} displayed a post/presurgical ratio of 4.36 (1.23–9.68). A fivefold increase in Q_{villi} resulted in a minor increase in AUC with a simulated post/pre-BPD-DS AUC ratio of 1.24 (0.22–3.24) and a C_{max} ratio of 1.86 (0.47–4.19). A reduction in GI CYP3A by fivefold gave a post/pre-BPD-DS AUC ratio of 1.13 (0.19–3.06) (**Figure 5**).

Pre to post-BPD-DS (SIT = 4.2 h) displayed an AUC ratio of 1.71 (0.74–5.79), C_{max} ratio of 1.56 (0.69–3.39), and a t_{max} ratio of 0.87 (0.51–1.31). In the sensitivity analysis, a twofold increase in Q_{villi} resulted in a post/presurgical AUC ratio of 2.07 (0.86–6.96) and a C_{max} ratio of 1.91 (0.84–4.22), whereas t_{max} remained unaltered. A twofold increase in P_{eff}

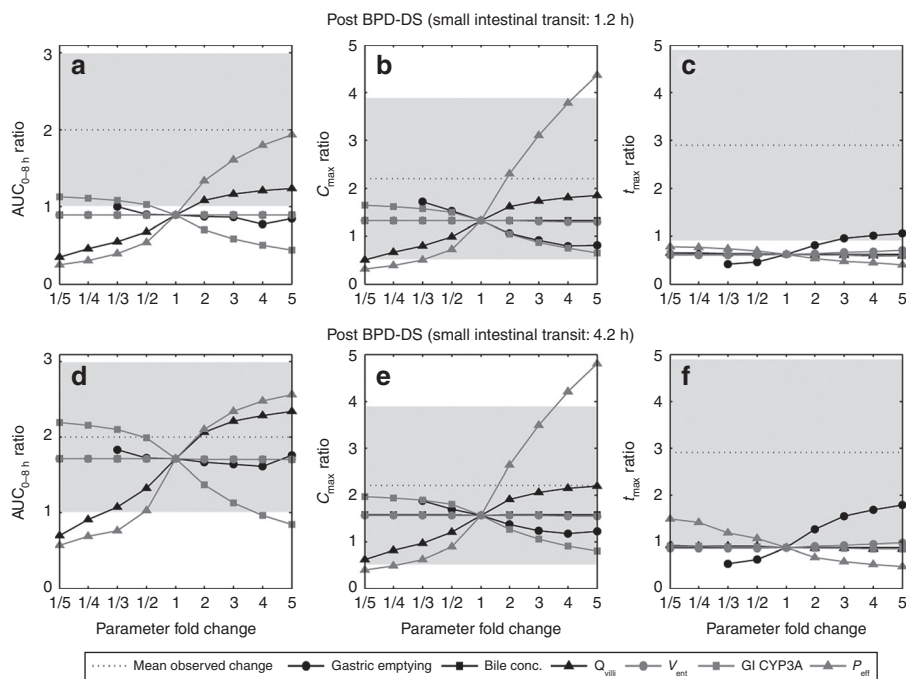


Figure 5 Spider plot of sensitivity analysis of simulated post/pre-biliopancreatic diversion with duodenal switch (BPD-DS) at a small intestinal transit time (SIT) of 1.2 h; (a) $AUC_{0-8 h}$, (b) C_{max} , and (c) t_{max} ratio, BPD-DS (SIT = 4.2 h); (d) $AUC_{0-8 h}$, (e) C_{max} , and (f) t_{max} ratio, examining the impact of the fold change in physiological parameters: gastric emptying, ileal bile concentration (bile conc.), villous blood flow (Q_{villi}), enterocytic volume (V_{ent}) in the remaining postsurgical small intestine, post-BPD-DS gastrointestinal CYP3A content, small intestinal permeability (P_{eff}), as compared with mean observed ratio pre- to post-BPD-DS.¹¹ AUC, area under the concentration–time curve; C_{max} , maximum plasma drug concentration; t_{max} , time of maximum plasma drug concentration.

displayed a post/pre-BPD-DS AUC ratio of 2.11 (0.90–6.91), a C_{max} ratio of 2.64 (1.17–5.66), and a minor reduction in t_{max} . A twofold reduction in GI CYP3A gave a post/presurgical AUC ratio of 1.99 (0.83–6.76), whereas C_{max} increased to a minor extent, displaying an AUC ratio of 1.80 (0.79–4.00). Gastric emptying had the most apparent impact on t_{max} , where a fivefold increase resulted in a post/pre-BPD-DS ratio of 1.78 (1.11–2.58) (Figure 5).

DISCUSSION

Cyclosporine

The immunosuppressant cyclosporine (molecular weight: 1202.61 g/mol) displays poor aqueous solubility and a relatively low permeability due to its lipophilic and bulky character making the compound dependent on bile-mediated solubility to facilitate absorption.^{23,24} The drug is mainly metabolized by CYP3A4 in the intestine and liver and is subject to P-glycoprotein efflux.^{25,26} The oral bioavailability displays a high interindividual variability, ranging from 5 to 89% for Sandimmune formulation, whereas Neoral displays improved absorption properties and an oral bioavailability of 21–73%.²⁷

The simulated underprediction of Sandimmune TDx trough levels before RYGB surgery was expected and is most likely due to the unspecificity of the immunoassay displaying a high cross-reactivity between the parent compound and metabolites resulting in a significantly higher variability in the trough levels as compared with peak concentrations.^{20,22}

Normalizing simulated cyclosporine trough levels to pre-RYGB levels produced a reduction in exposure comparable to observed data. Furthermore, a simulated 194% increase in Sandimmune dose levels recovered presurgical trough levels as stated in the publication.²⁰

In the simulation study of cyclosporine Neoral, microemulsion pre to post-JIB observed data of the control population was well described within the 95% prediction interval of the simulated data, whereas the observed exposure post-JIB was well described within the 95% prediction interval of simulated data assuming a reduction in SIT time equivalent to the bypass (SIT = 0.4 h). An alternative “what-if” scenario simulating a longer transit time (SIT = 0.7 h) over predicted the observed mean blood concentration post-JIB as reported by Chenhsu *et al.* (Figure 2). The overprediction could suggest small intestinal motility to remain unaltered following JIB or be a result of a small postsurgical study population ($n = 1$), displaying a low study power, albeit the simulated magnitude of reduction in C2 levels post-JIB (SIT = 0.4 h) closely matched the estimated reduction in cyclosporine exposure following JIB in another case study where a patient was subject to a surgical reversal of the procedure. The reversed JIB produced an observed 2.78-fold increase in exposure in the case study.^{21,28}

The simulated discrepancy in oral drug exposure of Sandimmune and Neoral pre to post-RYGB, where bariatric surgery had the highest effect on the oral bioavailability of Sandimmune, highlights the importance of formulation characteristics and its impact on oral drug bioavailability

pre- to post-bariatric surgery. The choice of a solubilized biopharmaceutical formulation such as a self-microemulsifying drug delivery system, solution, or dispersible tablet may be considered as a first-hand choice for patients undergoing bariatric surgery and are treated with limited solubility drugs with a narrow therapeutic index. This suggestion supports earlier observations in clinical practice, where alterations in pharmacotherapy post-bariatric surgery aim at switching to formulations displaying improved dissolution properties.⁵

Atorvastatin

The HMG-CoA reductase inhibitor atorvastatin, which is administered in the acid form, displays a high solubility and permeability. The compound is extensively metabolized in the small intestine and liver, namely by CYP3A4 but also via the UGT1A1 and UGT1A3 route. Atorvastatin acid and the lactone metabolite are also subject to interconversion by the UGTs and another minor chemical pathway. Atorvastatin acid is a substrate of P-glycoprotein efflux and OATP1B1-mediated active hepatic uptake.²⁹

Trends in simulated oral drug exposure of atorvastatin pre to post-RYGB were consistent with observed data, where simulated trends in f_a and F_g suggested an interplay between reduced absorption area and bypass of regions highly abundant in CYP3A to be of high importance when considering the overall effect on oral bioavailability. Simulated RYGB (SIT = 3.0 h) produced the closest agreement with observed data of atorvastatin exposure following RYGB, again suggesting a reduction in SIT time to be the most likely consequence of surgery.¹⁰

The inability to recover the observed twofold increase in atorvastatin AUC pre to post-BPD-DS at a simulated SIT of 1.2 h may suggest additional postsurgical physiological parameters to be governing the trend in oral drug bioavailability post-BPD-DS. The exploratory sensitivity analysis identified a number of potential parameters leading to a comparable increase in oral drug exposure pre to post-BPD-DS. An increase in SIT following BPD-DS, corresponding to the linear regression relationship between mouth to cecum transit time and plasma levels of peptide YY, resulted in an AUC ratio of 1.71 (0.74–5.79). Furthermore, a simulated twofold increase in P_{eff} and Q_{villi} , or a twofold reduction in the GI content of CYP3A post-BPD-DS (SIT = 4.2 h) recovered the observed AUC of atorvastatin. The reoccurring underprediction of t_{max} following surgery may be explained by an altered postprandial response causing a delayed absorption.

These findings suggest that additional physiological parameters, such as impairment in permeability or redistribution of intestinal blood flow, may play an important role in governing trends in oral drug exposure pre to immediately post-BPD-DS. The results highlight the surgery-specific trends observed post-bariatric surgery due to the intricate interplay between fluid dynamics, absorption area, transporters, metabolism, and GI physiology.

Current limitations in simulating the impact of oral drug bioavailability following bariatric surgery include the lack of clinical and postsurgical physiological data. Nonetheless, the models integrate all available knowledge on changes known to occur in the GI tract following bariatric surgery and can assist with dosage recommendation when there is an absence of clinical observations.

Table 1 Summary of alterations to population template in order to mimic and simulate postsurgical condition as per Darwich et al.⁶

Parameters	Bariatric surgical procedures			References
	JIB	RYGB	BPD-DS	
Gastric emptying: liquids (minutes)	24, ^a CV: 38%	7, CV: 45%	24, ^a CV: 38%	39,40
Gastric capacity (ml)	250 ^a	30	150	6,41
Q_{sec} stomach (l/h)	0.108	0.059	0.295	6
Initial volume of stomach fluid (ml)	50 ^a	9.9	32.6	6
Gastric pH	1.5 ^a	6.5	1.5 ^a	42–44
Small intestinal bypass (centimeters and/or segments)	Retaining the duodenum, 20% of jejunum I and 23% of ileum IV ^b	100 cm (duodenum and jejunum I) ^b	Retaining 2.5 cm of duodenum and 250 cm of the distal ileum ^c	6,41
Bile exclusion (centimeters and segments)	Not applicable (jejunum II – ileum III)	110 cm (stomach – jejunum I)	252 cm (stomach – ileum III)	6,41
CYP3A4 abundance (nmol/total gut)	32.3, CV: 60%	48.3, CV: 60%	12.6, ^d CV: 38%	6
CYP3A5 abundance (nmol/total gut)	12.1, CV: 60%	18.0, CV: 60%	10.1, ^d CV: 38%	6
Mean small intestinal transit time (hours) – Scenario 1	0.4; $\alpha = 0.5$, $\beta = 0.4$	3.0; $\alpha = 2.6$, $\beta = 3.7$	1.2; $\alpha = 1.3$, $\beta = 1.9$	6,41
Mean small intestinal transit time (hours) – Scenario 2	0.7; $\alpha = 0.6$, $\beta = 0.4$	5.0; $\alpha = 4.0$, $\beta = 5.3$	4.2; ^e $\alpha = 3.7$, $\beta = 5.0$	6,12,13,16
Renal equation	MDRD	MDRD	MDRD	6,45–48

ADAM, advanced dissolution absorption, and metabolism; BPD-DS, biliopancreatic diversion with duodenal switch; CV, coefficient of variation; JIB, jejunoileal bypass; MDRD, modification of diet renal disease equation; Q_{sec} , secretion flow; RYGB, Roux-en-Y gastric bypass; α and β , Weibull scaling factors utilizing assuming a variance of 1.8 h.

^aUnaltered parameter as compared with morbidly obese controls. ^bSetting human effective permeability (P_{eff}) of compounds close to zero in bypassed segments. ^cAltering small intestinal parameters in the ADAM model to conform to remaining segments. ^dBased on intestinal biopsy in the study population.¹¹

^eDerived based on a pre- to postsurgical peptide YY level of 413% utilizing linear relation between peptide YY and small intestinal transit time as reported by Savage and coworkers.^{16,18}

Conclusions

In this work, we demonstrated the potential of a PBPK and simulation to predict oral drug bioavailability post-bariatric surgery by evaluating earlier developed models using observed data for cyclosporine and atorvastatin. Trends in oral drug exposure of atorvastatin and cyclosporine were predicted well within the 95% prediction interval following RYGB using the previously developed model at a SIT time of 3.0 h. The results suggest a reduction in SIT time to be the most likely scenario following RYGB. The observed increase in atorvastatin exposure following BPD-DS could not be captured using the developed BPD-DS model incorporating all known physiological alterations.

A mechanistic PBPK modeling approach has the potential to serve as a tool in examining the impact of physiological alterations on oral drug bioavailability in the absence of clinical data. The demonstrated approach may allow a framework for optimization of oral drug therapy post-bariatric surgery.

METHODS

Bariatric surgery model. Sex-, age-, height-, and weight-matched simulations were carried out corresponding to identified clinical studies^{10,11,20,21} using the ADAM model coupled to a full PBPK distribution model, incorporated into the Simcyp Simulator (Simcyp, Sheffield, UK) (Eqs. 2–4).^{8,30} Detailed specification for the demographics and physiological parameters of the morbidly obese population have been published previously.⁷ Similarly, surgical changes to the anatomy and physiology of GI tract following bariatric surgeries, including: RYGB, BPD-DS, and JIB are defined in an earlier publication.⁶ Study population-specific surgical alterations are summarized in [Table 1](#).

$$\text{Height} = C0 + C1 \cdot \text{Age} + C2 \cdot \text{Age}^2 \quad (2)$$

$$\text{Weight} = e^{(C0 + C1 \cdot \text{Height})} \quad (3)$$

$$\text{BSA} = \text{Weight}^{\text{Weightexponent}} \cdot \text{Height}^{\text{Heightexponent}} \quad (4)$$

Cyclosporine. The cyclosporine compound file, available in the Simcyp Simulator compound library, was adapted to account for formulation properties corresponding to Sandimmune solution and Sandimmune Neoral microemulsion (Novartis, East Hanover, NJ), using an aqueous solubility of 0.01 mg/ml and particle sizes of 3.73 and 0.03 μm , respectively, further allowing Neoral to supersaturate freely without precipitation assuming a linear dose–concentration relationship.³¹ A full PBPK model was used to describe the cyclosporine distribution, where tissue to plasma partition coefficients (Kps) were obtained from *in vivo* tissue to plasma concentrations at steady state following intravenous infusion in rat.³²

Atorvastatin acid. Physicochemical parameters for atorvastatin acid were taken from the publication by Lennernäs.²⁹ Metabolic data were obtained from the *in vitro* study reported by Jacobsen *et al.*³³ CYP3A4 was found to be the main enzyme involved in the formation of the two primary metabolites ortho- and para-hydroxyatorvastatin acid with a minor contribution from CYP2C8. Intersystem extrapolation factors,

which correct for differences in intrinsic activity per unit CYP enzyme relative to its native environment, were applied to the kinetic data for recombinantly expressed CYP3A4 and CYP2C8, respectively. Acyl glucuronidation of atorvastatin acid to the lactone and UDPGA-dependent metabolism of atorvastatin acid mainly via UGT1A1 to a minor ether glucuronide was also considered.^{34,35} The resultant intrinsic clearance data were scaled to whole-organ values according to Eqs. 5 and 6.³⁶ The uptake of atorvastatin acid has been demonstrated in an OATP1B1-transfected cell system (HEK293 cells).^{37,38} Although these *in vitro* data support the involvement of OATP1B1 in the hepatic uptake of atorvastatin acid, it was found that when used in combination with the metabolic data, the clearance was significantly underpredicted. To recover the plasma concentration time profile of atorvastatin acid before BPD-DS, $J_{\text{max, OATP1B1}}$ and $K_{\text{p, muscle}}$ were reestimated to 532.4 pmol/min/million cells and 4.0, using weighted least-square Nelder–Mead minimization method in the parameter estimation toolbox within the Simcyp Simulator.¹¹

$$CL_{U_{H, \text{int}}} = \frac{\text{ISEF} \cdot V_{\text{max-rhCYP}} \cdot \text{Abundance} \cdot \text{MPPGL} \cdot \text{Liver Weight}}{K_{m,u}} \quad (5)$$

$$CL_{U_{G, \text{int}}} = \frac{\text{ISEF} \cdot V_{\text{max-rhCYP}} \cdot \text{Abundance}}{K_{m,u}} \quad (6)$$

Sensitivity analysis was carried out with regard to potential GI physiological parameters subject to potential alterations following surgery due to hormonal alterations, including: SIT time, villous blood flow (Q_{villi}), gastric emptying, small intestinal bile concentration, the enterocyte volume in the remaining small intestine (V_{ent}), postsurgical abundance of GI CYP3A (GI CYP3A), and small intestinal effective permeability (P_{eff}).

Analysis. Simulated data were visually inspected against observed data. In addition, the potential mechanism of changes to oral drug absorption was examined through the simulations in terms of assessing the effects on plasma drug concentration–time profile, maximum plasma drug concentration (C_{max}), time of maximum plasma drug concentration (t_{max}), f_a , and F_G .

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Conflict of interest. D.P., K.R.-Y., and M.J. are employees in Simcyp Limited (a Certara Company). A.R.-H. is an employee of the University of Manchester and part-time secondee to Simcyp Limited (a Certara Company). The other authors declared no conflict of interest.

Study Highlights

WHAT IS THE CURRENT KNOWLEDGE?

- ✓ Patients undergoing bariatric surgery receive various therapeutic drugs. A limited number of studies have investigated oral drug exposure postoperatively. Bariatric surgery models were previously developed using the ADAM model within the PBPK simulator, Simcyp.

WHAT QUESTION THIS STUDY ADDRESSED?

- ✓ We report on the evaluation of previously developed bariatric surgery PBPK models by comparing observed vs. predicted impact of surgery on oral exposure of cyclosporine and atorvastatin.

WHAT THIS STUDY ADDS TO OUR KNOWLEDGE

- ✓ Trends in oral exposure of atorvastatin and cyclosporine were well predicted following RYGB. Observed increase in atorvastatin exposure following BPD-DS could not be captured using the current model.

HOW THIS MIGHT CHANGE CLINICAL PHARMACOLOGY AND THERAPEUTICS

- ✓ The potential of a PBPK modeling approach was demonstrated, allowing a framework for optimizing oral drug therapy post-bariatric surgery. Developed models integrated available knowledge on physiological changes. The study highlights areas of further research, where models are not predictive due to the lack of information on systems parameters.

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Supplementary information accompanies this paper on the *Pharmacometrics & Systems Pharmacology* website (<http://www.nature.com/psp>)

8.3.2 Compound Simcyp Simulator template input properties

Table 8.4. Drug specific parameters for atorvastatin acid.

Parameters	Value	References
PhysChem		
MW (g/mol)	546	(NCBI, 2011)
LogP _{o:w}	4.47	(Lennernas, 2003)
Acid-base nature	Acid	
pKa	4.46	
Blood binding		
BP	0.61	(Watanabe <i>et al.</i>)
fu _p	0.02	(Gibson, 1997)
Dissolution		
Solubility input	Measured	(Lennernas, 2003)
Aqueous solubility, pH 6 (mg/mL)	1.23	
Particle size (µm)	10	
Absorption		
Caco-2 pH7.4:7.4 (10 ⁻⁴ cm/s)	P _{app} : 7.9 (P _{eff,man} : 4.9)	(Wu <i>et al.</i> , 2000)
Distribution		
V _{ss} (L/kg)	4.76	(Gibson, 1997)
Distribution model	Full PBPK	
Prediction method	Rodgers <i>et al.</i>	(Rodgers <i>et al.</i> , 2005; Rodgers and Rowland, 2006)
Metabolism		
<i>rCYP2C8: Para-OH</i>		(Jacobsen <i>et al.</i> , 2000)
CL _{int} (µL/min/mg protein)	4.5	
V _{max} (pmol/min/pmol CYP)	0.29	
K _m (µM)	35.9	
ISEF	0.98	
<i>rCYP3A4: Para-OH</i>		
CL _{int} (uL/min/mg protein)	219	
V _{max} (pmol/min/pmol CYP)	29.8	
K _m (µM)	25.6	
ISEF	0.24	
<i>rCYP3A4: Ortho-OH</i>		
CL _{int} (µL/min/mg protein)	184	
V _{max} (pmol/min/pmol CYP)	29.3	
K _m (µM)	29.7	
ISEF	0.24	
<i>UGT1A1</i>		
CL _{int} (µL/min/mg protein)	5.23	
Acyl glucuronidation (Lactonisation)		
CL _{int} (µL/min/mg protein)	7.22	
<i>Non-UGT</i> (Lactonisation)		
CL _{int} (µL/min/mg protein)	200	
Transport		
<i>P-glycoprotein</i> (ABCB1; Apical efflux, intestine)		(Wu <i>et al.</i> , 2000)
J _{max} (pmol/min)	141 ^B	
K _m (µM)	115	
<i>OATP1B1</i> (SLCO1B1; Sinusoidal uptake, liver)		(Lau <i>et al.</i> , 2007; Amundsen <i>et al.</i> , 2010)
J _{max} (pmol/min/10 ⁶ hepatocytes)	1612 ^B	
K _m (µM)	0.93	

BP =Blood to plasma ratio, fu_p=fraction unbound in plasma, ISEF=Inter System Extrapolation Factor, CL_{pd}=Passive diffusion clearance.

^APredicted from Caco-2 permeability data.

^BDerived utilising the parameter estimation toolbox within the Simcyp Simulator based on 12 healthy volunteers receiving atorvastatin acid 40 mg (Lilja *et al.*, 1999).

Table 8.5. Drug specific parameters for cyclosporine.

Parameters	Value	References
PhysChem		
MW (g/mol)	1202	(Turner, 2008; NCBI, 2011)
LogP _{o:w}	4.3	
Acid-base nature	Neutral	
pKa	NA	
Blood binding		
BP	1.36	(Turner, 2008)
f _{u,p}	0.037	
Dissolution		
Sandimmune		(Andrysek, 2003; Persson <i>et al.</i> , 2005)
Solubility method	Human intestinal fluids	
Solubility (mg/mL)	0.011	
Particle Size (um)	1.84	
Supersaturation ratio	10	
Neoral		
Solubility method	Human intestinal fluids	
Solubility (mg/mL)	0.011	
Particle Size (um)	0.018	
Supersaturation ratio	1000	
Absorption		
P _{eff,man}	1.65	(Turner, 2008)
Distribution		
V _{ss} (L/kg)	5.6	(Bernareggi and Rowland, 1991)
Distribution model	Full PBPK	
Prediction method	Rat Kp's, measured.	
Metabolism		
CYP3A4		(Turner, 2008)
CL _{int} (uL/min/mg protein)	219	
V _{max} (pmol/min/mg microsomal protein)	29.8	
K _m (uM)	25.6	

BP =Blood to plasma ratio, fu_p=fraction unbound in plasma, P_{eff,man}=effective human jejunal permeability, V_{ss}=Volume of distribution at steady state following intravenous infusion.

8.3.3 Supplementary results

Simulated oral drug bioavailability of cyclosporine (Neoral[®]) post Roux-en-Y gastric bypass (Figure 8.1).

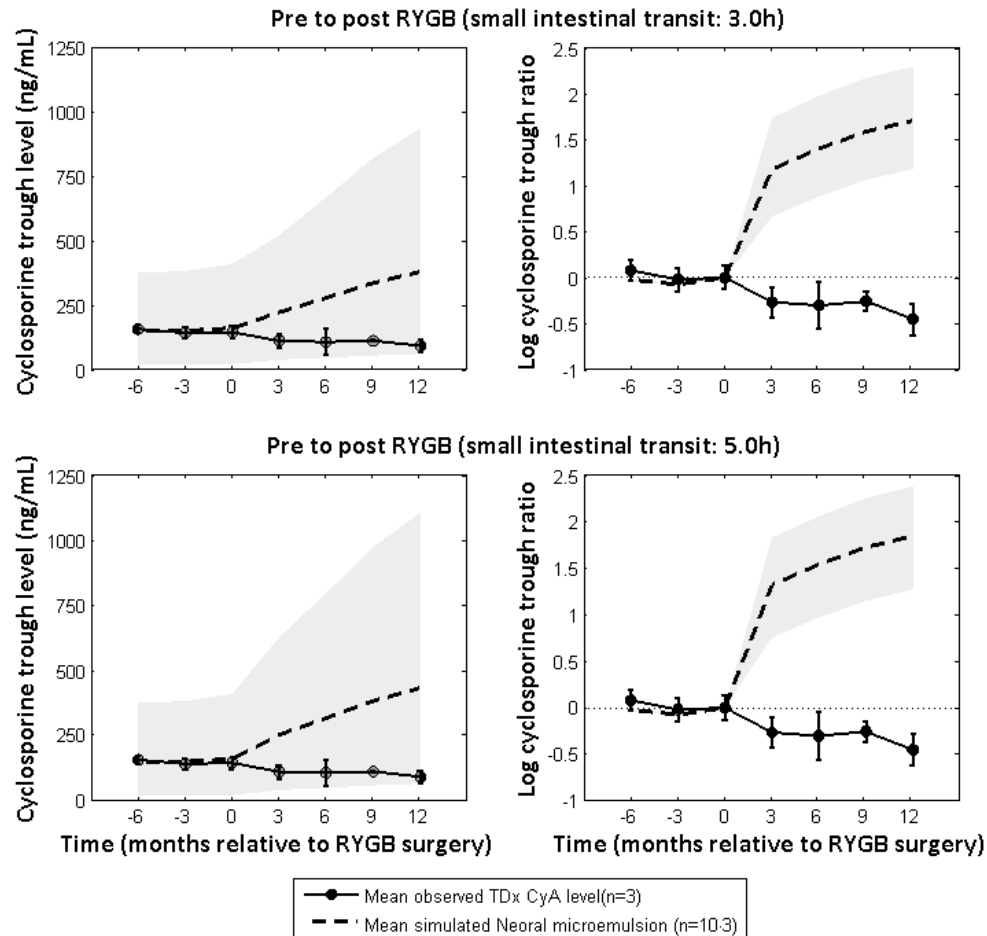


Figure 8.1. Mean and standard deviation of observed cyclosporine (CsA) TDx trough levels at steady state pre to post Roux-en-Y gastric bypass (RYGB) at -6, -3, 0, 3, 6, 9 and 12 months relative to RYGB surgical event (0 months). Time points from -6 to 12 months correspond to dose levels of: 1.7, 1.7, 1.8, 2.4, 2.8, 3.2, 3.5 mg/kg/day respectively (n patients=3) administered twice daily. Observed data is compared to simulated 50, 95 and 5% prediction interval, indicated by grey area, of cyclosporine Neoral[®] trough levels (n patients=10.3), A: Simulated post RYGB at a small intestinal transit time (SIT) of 3.0h, B: Log normalised simulated CsA trough ratio as compared to 0 months (RYGB SIT=3.0h), C: Simulated CsA trough levels at RYGB SIT of 5.0h, D: Log normalised simulated CsA trough ratio as compared to 0 months (RYGB SIT=5.0h) (Marterre *et al.*, 1996).

Simulated oral drug bioavailability of cyclosporine (Neoral[®]) post jejunoileal bypass at a small intestinal transit time of 0.7h (Figure 8.2).

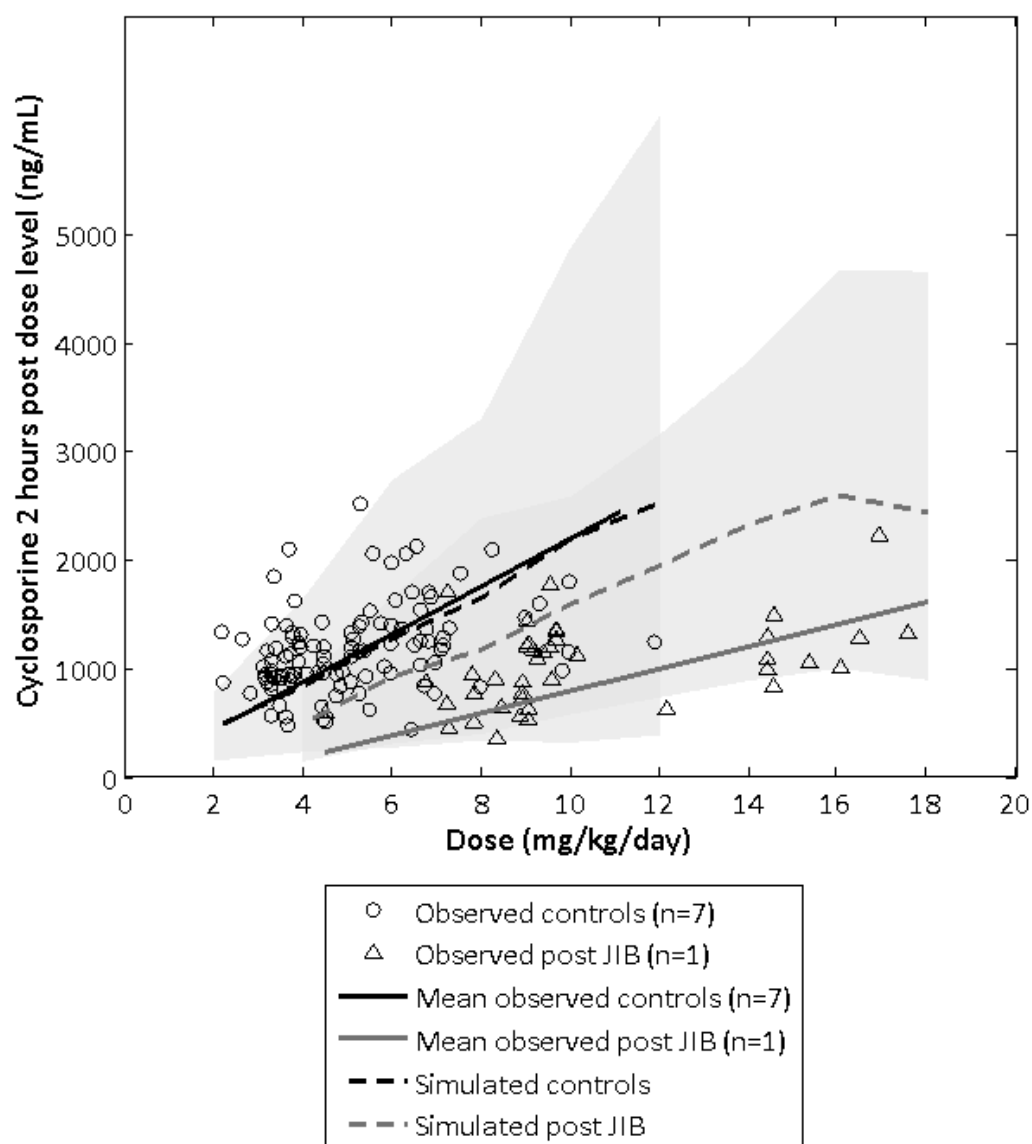


Figure 8.2. Observed mean blood concentration of cyclosporine microemulsion (Sandimmune[®] Neoral[®], Novartis) at steady state 2 hours post dosing in controls (n=7) and one patient (n=1) post jejunoileal bypass (JIB) as compared to simulated sex and age matched controls (n=300) and post JIB (n patients=800) at a small intestinal transit time of 0.7 hours over dose range of 300 to 1,000 mg including, where 5, 50 and 95% prediction intervals are indicated by grey areas (Chenhsu *et al.*, 2003).

Simulated oral drug bioavailability of atorvastatin post Roux-en-Y gastric bypass at a small intestinal transit time of 5.0h (Figure 8.3).

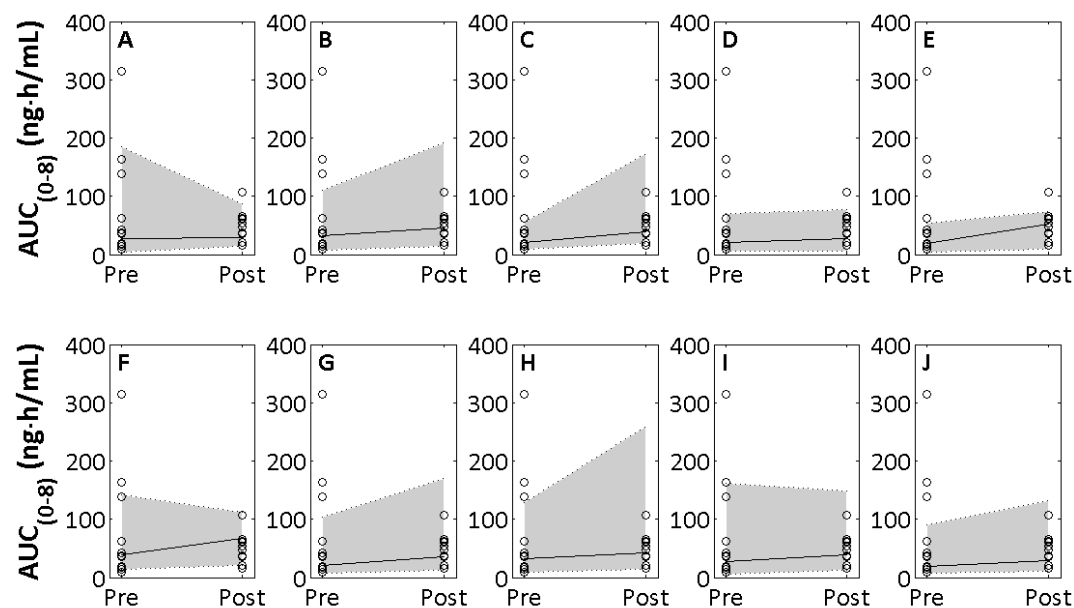


Figure 8.3. Simulated 50, 95 and 5% prediction interval (indicated by grey areas) of oral drug exposure of atorvastatin acid in randomised trials of age, sex, dose and BMI (Body Mass Index) matched patients pre to post Roux-en-Y gastric bypass surgery (small intestinal transit=5.0h) as compared to observed data A-J: Ten randomised simulated trials consisting of 10 individuals in each trial (n individuals=10-12), as compared to observed ($n=12$; \circ) (Skottheim *et al.*, 2009).

Simulated oral drug bioavailability of atorvastatin acid in morbidly obese prior to biliopancreatic diversion with duodenal switch as compared to observed, utilising visual predictive check (VPC) (Skottheim *et al.*, 2010).

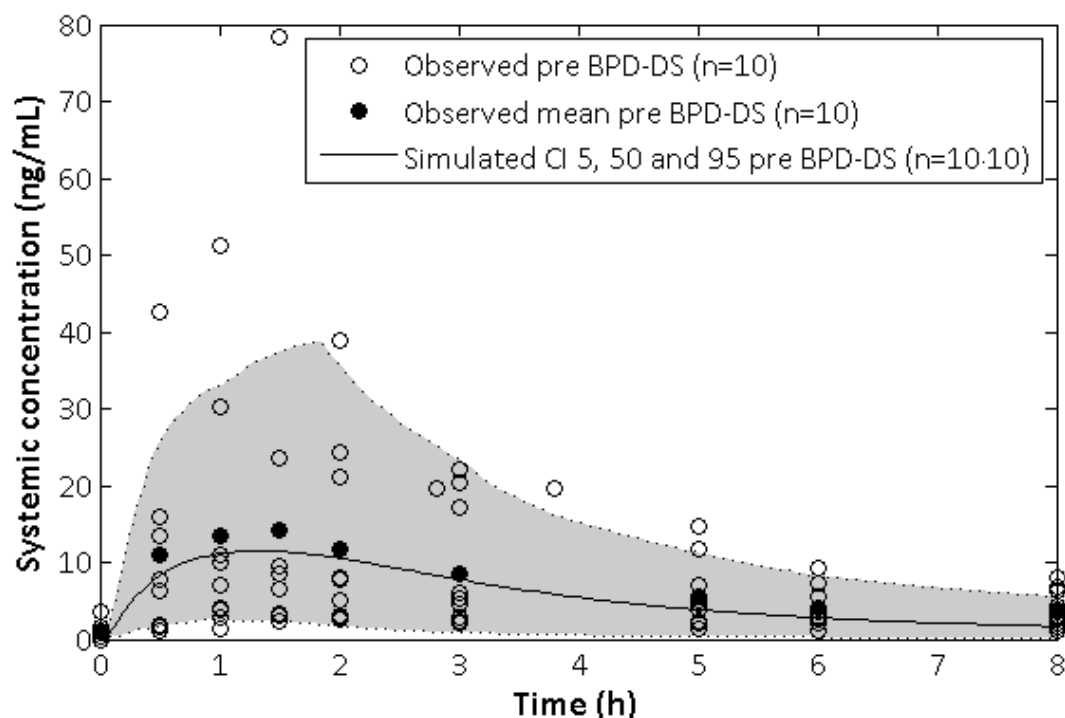


Figure 8.4. Age, sex, weight and dose matched simulated mean, 95th and 5th percentile of systemic plasma concentration of atorvastatin acid following orally administered atorvastatin acid immediate release (IR) 20-80 mg (n individuals=10:10) as compared to observed data (n=10) (Skottheim *et al.*, 2010).

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8.4 Assessing the turnover of the intestinal epithelia in pre-clinical species and human

8.4.1 Supplementary enterocyte turnover data in pre-clinical species and human

Table 8.6. Enterocyte turnover in the small intestine of the mouse.

Segment	Turnover (days)	SD	N	Method	References
Duodenum	2.81	0.23	16	H-Thymidine, <i>in vivo</i>	(Ferraris <i>et al.</i> , 1992)
Duodenum	3.09	0.31	16	H-Thymidine, <i>in vivo</i>	(Ferraris <i>et al.</i> , 1992)
Duodenum	2.43	0.13	NA	H-Thymidine, <i>in vivo</i>	(Cheng and Bjerknes, 1982)
Duodenum	2.35	0.56	5	H-Thymidine, <i>in vivo</i>	(Merzel and Leblond, 1969)
Duodenum	3.3	NA	8	H-Thymidine, <i>in vivo</i>	(Cheng and Leblond, 1974)
Duodenum	2	NA	1	H-Thymidine, <i>in vivo</i>	(Walker and Leblond, 1958)
Duodenum	2.08	NA	6	H-Thymidine, <i>in vivo</i>	(Grey, 1968)
Duodenum	1.71	NA	20	H-Thymidine, <i>in vivo</i>	(Leshner <i>et al.</i> , 1961)
Duodenum	2	NA	20	H-Thymidine, <i>in vivo</i>	(Leshner <i>et al.</i> , 1961)
Duodenum	2.21	NA	20	H-Thymidine, <i>in vivo</i>	(Leshner <i>et al.</i> , 1961)
Jejunum	3.17	0.33	16	H-Thymidine, <i>in vivo</i>	(Ferraris <i>et al.</i> , 1992)
Jejunum	2.85	0.31	16	H-Thymidine, <i>in vivo</i>	(Ferraris <i>et al.</i> , 1992)
Jejunum	2.59	0.18	NA	H-Thymidine, <i>in vivo</i>	(Cheng and Bjerknes, 1982)
Jejunum	3.4	NA	8	H-Thymidine, <i>in vivo</i>	(Cheng and Leblond, 1974)
Jejunum	4	NA	20	H-Thymidine, <i>in vivo</i>	(Thompson <i>et al.</i> , 1990)
Jejunum	1.83	NA	34	H-Thymidine, <i>in vivo</i>	(Fry <i>et al.</i> , 1961)
Jejunum	2.17	NA	34	H-Thymidine, <i>in vivo</i>	(Fry <i>et al.</i> , 1961)
Jejunum	2.21	NA	52	H-Thymidine, <i>in vivo</i>	(Fry <i>et al.</i> , 1961)
Ileum	2.6	0.38	16	H-Thymidine, <i>in vivo</i>	(Ferraris <i>et al.</i> , 1992)
Ileum	2.56	0.35	16	H-Thymidine, <i>in vivo</i>	(Ferraris <i>et al.</i> , 1992)
Ileum	2.43	0.12	NA	H-Thymidine, <i>in vivo</i>	(Cheng and Bjerknes, 1982)
Ileum	2	NA	NA	H-Thymidine, <i>in vivo</i>	(Quastler and Sherman, 1959)
Ileum	1.29	NA	10	H-Thymidine, <i>in vivo</i>	(Fry <i>et al.</i> , 1962)
Ileum	1.38	NA	8	H-Thymidine, <i>in vivo</i>	(Fry <i>et al.</i> , 1962)
Ileum	1.29	NA	10	H-Thymidine, <i>in vivo</i>	(Fry <i>et al.</i> , 1962)
Jejunum and ileum	3	NA	NA	H-Thymidine, <i>in vivo</i>	(Leblond and Messier, 1958)
NA	2.67	NA	7	H-Thymidine, <i>in vivo</i>	(Smith <i>et al.</i> , 1984)

NA=Not applicable.

Table 8.7. Enterocyte turnover in the small intestine of the rat.

Segment	Turnover (days)	SD	N	Method	References
Proximal SI	1.24	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Proximal SI	1.97	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Proximal SI	1.71	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Proximal SI	2.01	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Proximal SI	1.86	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Duodenum	1.57	NA	4	Histological study	(Leblond and Stevens, 1948)
Duodenum	1.2	0.2	4	C-glycoside, <i>in vivo</i>	(Macallan <i>et al.</i> , 1998)
Duodenum	1.59	NA	5	BrdUrd, <i>in vivo</i>	(Qi <i>et al.</i> , 2009)
Duodenum	1.78	NA	12	H-Thymidine, <i>in vivo</i>	(Holt <i>et al.</i> , 1983)
Duodenum	1.98	NA	12	H-Thymidine, <i>in vivo</i>	(Holt <i>et al.</i> , 1983)
Duodenum	2.5	NA	8	H-Thymidine, <i>in vivo</i>	(Loran and Althausen, 1960)
Duodenum	2.22	NA	6	H-Thymidine, <i>in vivo</i>	(Koldovsky <i>et al.</i> , 1966)
Median SI	2.07	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Median SI	2.3	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Median SI	1.88	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Median SI	1.68	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Median SI	1.44	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Proximal jejunum	1.5	NA	5	BrdUrd, <i>in vivo</i>	(Qi <i>et al.</i> , 2009)
Jejunum	2.29	NA	6	H-Thymidine, <i>in vivo</i>	(Thomson <i>et al.</i> , 1994)
Jejunum	2.21	NA	8	H-Thymidine, <i>in vivo</i>	(Thomson <i>et al.</i> , 1994)
Jejunum	1.54	NA	6	H-Thymidine, <i>in vivo</i>	(Thomson <i>et al.</i> , 1994)
Jejunum	2.33	NA	6	H-Thymidine, <i>in vivo</i>	(Thomson <i>et al.</i> , 1994)
Jejunum	2.25	NA	7	H-Thymidine, <i>in vivo</i>	(King <i>et al.</i> , 1983)
Jejunum	2.38	NA	7	H-Thymidine, <i>in vivo</i>	(King <i>et al.</i> , 1983)
Jejunum	2.04	NA	3	H-Thymidine, <i>in vivo</i>	(Cheeseman, 1986)
Jejunum	1.3	NA	NA	NA	(Bertalanffy and Lau, 1962)
Jejunum	2.06	NA	12	H-Thymidine, <i>in vivo</i>	(Holt <i>et al.</i> , 1983)
Jejunum	2.2	NA	12	H-Thymidine, <i>in vivo</i>	(Holt <i>et al.</i> , 1983)
Jejunum	2.08	NA	8	H-Thymidine, <i>in vivo</i>	(Loran and Althausen, 1960)
Jejunum	2.22	NA	6	H-Thymidine, <i>in vivo</i>	(Koldovsky <i>et al.</i> , 1966)
Jejunum	3.94	0.54	10	H-Thymidine, <i>in vivo</i>	(Shambaugh <i>et al.</i> , 1967)

Jejunum	1.3	NaN	16	Colchine technique, <i>in vivo</i>	(Bertalanffy, 1960)
Distal jejunum	1.64	NA	5	BrdUrd, <i>in vivo</i>	(Qi <i>et al.</i> , 2009)
Distal SI	2.5	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Distal SI	3.05	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Distal SI	2.7	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Distal SI	2.48	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Distal SI	1.45	NA	2	H-Thymidine, <i>in vivo</i>	(Menge <i>et al.</i> , 1982)
Proximal ileum	1.62	NA	5	BrdUrd, <i>in vivo</i>	(Qi <i>et al.</i> , 2009)
Ileum	1.88	NA	6	H-Alanine and lysine uptake	(Menge <i>et al.</i> , 1983)
Ileum	1.35	NA	4	Histological study	(Leblond and Stevens, 1948)
Ileum	1.64	NA	12	H-Thymidine, <i>in vivo</i>	(Holt <i>et al.</i> , 1983)
Ileum	1.37	NA	12	H-Thymidine, <i>in vivo</i>	(Holt <i>et al.</i> , 1983)
Ileum	1.6	NA	25	Vincristine, <i>in vivo</i>	(Alam <i>et al.</i> , 1994)
Ileum	2.82	NA	8	H-Thymidine, <i>in vivo</i>	(Loran and Althausen, 1960)
Ileum	2.5	NA	6	H-Thymidine, <i>in vivo</i>	(Koldovsky <i>et al.</i> , 1966)
Distal ileum	1.43	NA	5	BrdUrd, <i>in vivo</i>	(Qi <i>et al.</i> , 2009)
NA	2.1	NA	5	Colchine technique, <i>in vivo</i>	(Altmann and Enesco, 1967)

NA=Not applicable, SI=Small intestine.

Table 8.8. Enterocyte turnover in the human gastrointestinal tract.

Segment	Turnover (Days)	SD	N	Method	References
Oesophagus	6.35	2.08	1	H-Thymidine, <i>in vivo</i>	(Bell <i>et al.</i> , 1967)
Stomach	5	1	2	H-Thymidine, <i>in vivo</i>	(Macdonald <i>et al.</i> , 1964)
Stomach	3.5	0.5	3	H-Thymidine, <i>in vivo</i>	(Lipkin <i>et al.</i> , 1963b)
Stomach	3.46	1.21	16	BrdUrd, <i>in vivo</i>	(Patel <i>et al.</i> , 1993)
Stomach	2.58	1.17	10	BrdUrd, <i>in vivo</i>	(Patel <i>et al.</i> , 1993)
Stomach	3.43	1.14	4	H-Thymidine, <i>in vivo</i>	(Wright <i>et al.</i> , 1977)
Duodenum	5.42	NA	1	H-Thymidine, <i>in vivo</i>	(Macdonald <i>et al.</i> , 1964)
Duodenum	5.5	0.5	1	H-Thymidine, <i>in vivo</i>	(Macdonald <i>et al.</i> , 1964)
Duodenum	2	NA	56	Histological study	(Bertalanffy and Nagy, 1961)
Duodenum	1.26	0.17	2	H-Thymidine, <i>in vivo</i>	(Weinstein, 1974)
Jejunum	5	NA	3	H-Thymidine, <i>in vivo</i>	(Shorter <i>et al.</i> , 1964)
Ileum	1.4	NA	6	Histological study	(Bullen <i>et al.</i> , 2006)
Ileum	3	NA	3	H-Thymidine, <i>in vivo</i>	(Lipkin <i>et al.</i> , 1963b)
Colon	1	NA	2	H-Thymidine, <i>in vivo</i>	(Lipkin <i>et al.</i> , 1963a)
Colon	0.83	NA	3	H-Thymidine, <i>in vivo</i>	(Lipkin <i>et al.</i> , 1963b)
Colon	3.41	NA	66	BrdUrd, <i>in vivo</i>	(Potten <i>et al.</i> , 1992)
Colon	1.63	NA	1	H-Thymidine, <i>in vivo</i>	(Lipkin, 1969)
Colon	3.04	0.25	8	H-Thymidine, <i>in vitro</i>	(Bleiberg and Galand, 1976)
Rectum	5.5	0.5	2	H-Thymidine, <i>in vivo</i>	(Macdonald <i>et al.</i> , 1964)
Rectum	7	1	1	H-Thymidine, <i>in vivo</i>	(Cole and Mc, 1961)
Rectum	3.66	0.42	18	Histological study	(Shorter <i>et al.</i> , 1966)
Rectum	4.73	0.59	9	Histological study	(Shorter <i>et al.</i> , 1966)
Rectum	5.45	0.61	17	Histological study	(Shorter <i>et al.</i> , 1966)
Rectum	0.83	NA	3	H-Thymidine, <i>in vivo</i>	(Lipkin <i>et al.</i> , 1963b)
Rectum	3	NA	3	H-Thymidine, <i>in vivo</i>	(Shorter <i>et al.</i> , 1964)
Rectum	3.5	0.5	16	H-Thymidine, <i>in vitro</i>	(Deschner <i>et al.</i> , 1963)
Rectum	3.75	NA	8	H-Thymidine, <i>in vitro</i>	(Bleiberg <i>et al.</i> , 1970)

NA=Not applicable

8.4.2 References

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8.5 Development and assessment of a nested enzyme-within-enterocyte turnover model for mechanism-based inhibition in the small intestine

8.5.1 Supplementary data for sensitivity analysis

Table 8.10. Dose levels and observed absorption rate constants (k_a) of drugs included in the 17th WHO model list of Essential Medicines.

Drugs	Low dose (μmoles)*	Medium dose (μmoles)*	High dose (μmoles)*	(h^{-1})	References
Abacavir		1047.73		1.65	(Weller <i>et al.</i> , 2000)
Acetazolamide		1124.88		0.82	(Yano <i>et al.</i> , 1998)
Acetylsalicylic acid	555.07		2775.35	0.85	(Iiaz <i>et al.</i> , 2003)
Albendazole		1507.55		1.41	(Cotting <i>et al.</i> , 1990)
Allopurinol	734.69		2204.08	1.64	(Turnheim <i>et al.</i> , 1998)
Amiloride		21.77		1.77	(Savic <i>et al.</i> , 2007)
Amiodarone	154.96	309.93	619.86		
Amitriptyline		90.12		0.41	(Kukes <i>et al.</i> , 2009)
Amlodipine		12.23		0.79	(Flynn <i>et al.</i> , 2006)
Amodiaquine	189.68	379.36	758.72	1.41	(Jullien <i>et al.</i> , 2010)
Amoxicillin	684.17		1368.35	0.79	(Arancibia <i>et al.</i> , 1998)
Artemether		67.03		1.41	(Ezzet <i>et al.</i> , 2008)
Atazanavir	141.87	212.81	425.62	1.02	(Solas <i>et al.</i> , 2008)
Azathioprine		180.33			
Benznidazole		384.25			
Biperiden	6.42	6.42	6.42		
Bisoprolol	3.84		15.36		
Caffeine				2.36	(Kamimori <i>et al.</i> , 1985)
Carbamazepine	423.25		846.49	0.29	(Ismail and Rahman, 1985)
Cefixime		882.13		0.35	(Brittain <i>et al.</i> , 1985)

Additional references: (BNF, 2011; PubChem, 2011; WHO, 2011)

Table 8.10. Dose levels and observed absorption rate constants (k_a) of drugs included in the 17th WHO model list of Essential Medicines.

Drugs	Low dose (μmoles)*	Medium dose (μmoles)*	High dose (μmoles)*	k_a (h^{-1})	References
Chloramphenicol	773.68				
Chloroquine	312.62		468.94	1.40	(Karunajeewa <i>et al.</i> , 2010)
Chlorpromazine	31.36	117.60	313.61	0.53	(Whitfield <i>et al.</i> , 1978)
Ciprofloxacin		754.51		2.70	(Sanchez Navarro <i>et al.</i> ,
Clarithromycin		668.49		0.56	(Abduljalil <i>et al.</i> , 2009)
Clofazimine	105.62		211.24	0.99	(Nix <i>et al.</i> , 2004)
Clomipramine	31.76		79.40		
Cloxacillin	1147.10		2294.20		
Codeine		100.21			
Cyclizine		187.70		1.54	(Walker, 1995)
Cyclophosphamide		95.75			
Dapsone	100.68	201.37	402.74	0.93	(Simpson <i>et al.</i> , 2006)
Dexamethasone		5.10			
Diazepam	7.02	17.56	35.12		
Didanosine	105.83	423.32	846.64	1.51	(Velasque <i>et al.</i> , 2007)
Diethylcarbamazine	25.09		50.18	2.23	(Bolla <i>et al.</i> , 2002)
Digoxin	0.01		0.32		
Diloxanide		2136.03			
Doxycycline	112.50		225.01		
Efavirenz	1900.69	1900.69	1900.69	1.39	(Pfister <i>et al.</i> , 2003)

Additional references: (BNF, 2011; PubChem, 2011; WHO, 2011)

Table 8.10. Dose levels and observed absorption rate constants (k_a) of drugs included in the 17th WHO model list of Essential Medicines.

Drugs	Low dose (μmoles)*	Medium dose (μmoles)*	High dose (μmoles)*	k_a (h^{-1})	References
Emitricitabine		808.91		0.54	(Hirt <i>et al.</i> , 2009)
Enalapril	6.64		13.28		
Erythromycin		340.63			
Ethambutol	489.45	1346.00	1957.81	0.47	(Jonsson <i>et al.</i> , 2011)
Ethinyl	0.10		0.12		
Ethosuximide		1770.94			
Ferrous		394.98		1.29	(Farheen <i>et al.</i> , 2002)
Fluconazole		163.25			
Fludrocortisone		0.26			
Fluoxetine		64.66			
Folic acid	0.91	2.27	11.33		
Furosemide	30.23	60.47	120.94		
Glibenclamide	5.06		10.12		
Griseofulvin	354.34		708.68		
Haloperidol	5.32		13.30		
Hydralazine	156.08		312.16		
Hydroxycarbamide	2629.69	4766.31	13148.44	3.29	(Paule <i>et al.</i> , 2011)
Hydrochlorothiazide	41.98		83.97	0.31	(Beermann and
Ibuprofen	969.55	1939.10	2908.66		
Indinavir		651.69		1.50	(Pfister <i>et al.</i> , 2003)

Additional references: (BNF, 2011; PubChem, 2011; WHO, 2011)

Table 8.10. Dose levels and observed absorption rate constants (k_a) of drugs included in the 17th WHO model list of Essential Medicines.

Drugs	Low dose (μmoles)*	Medium dose (μmoles)*	High dose (μmoles)*	k_a (h^{-1})	References
Isoniazid	364.59	729.19	2187.56	1.85	(Wilkins <i>et al.</i> , 2011)
Ivermectin	3.43		6.86	0.24	(El-Tahtawy <i>et al.</i> ,
Lactulose	135.85		540.47		
Lamivudine	130.86		654.29	4.65	(Moore <i>et al.</i> , 1999)
Levamisole	244.75		734.25		
Levodopa	507.13		1267.83	3.38	(Triggs <i>et al.</i> , 1996)
Levonorgestrel	0.10	2.40	4.80		
Levothyroxine	0.03	0.06	0.13		
Lithium		4060.04			
Lopinavir	159.03	211.99	318.07	0.26	(Dickinson <i>et al.</i> ,
Lumefantrine		226.87		0.13	(Ezzet <i>et al.</i> , 1998)
Mebendazole	338.65		1693.24		
Medroxyprogesterone		12.94			
Mefloquine		660.83			
Mesna	2436.36		3654.55		
Metformin		3871.06		0.51	(Bardin <i>et al.</i> , 2012)
Methadone	16.16		32.32	0.39	(Rostami-Hodiegan <i>et</i>
Methotrexate		5.50		1.11	(Hoekstra <i>et al.</i> , 2006)
Mehtyldopa		1183.63			
Metoclopramide		33.36			

Additional references: (BNF, 2011; PubChem, 2011; WHO, 2011)

Table 8.10. Dose levels and observed absorption rate constants (k_a) of drugs included in the 17th WHO model list of Essential Medicines.

Drugs	Low dose (μmoles)*	Medium dose (μmoles)*	High dose (μmoles)*	k_a (h^{-1})	References
Metronidazole	1168.54		2921.35		
Midazolam	23.02		46.05	2.20	(Gertz <i>et al.</i> , 2011)
Mifepristone		465.56			
Miltefosine	24.54		122.68	0.42	(Dorlo <i>et al.</i> , 2012)
Misoprostol	0.52	0.52	0.52		
Neostigmine		67.18			
Nevirapine	187.76	375.52	751.04	1.68	(de Maat <i>et al.</i> , 2002)
Niclosamide		1528.49			
Nicotine	12.33	409.42		3.79	(Strafford <i>et al.</i> , 1996)
Nifedipine			24.66		
Nitrofurantoin	104.42	28.87		2.22	(Ahmad <i>et al.</i> , 2009)
Nitrofurantoin		417.69	870.19	0.97	(Garcia-Bournissen <i>et</i>
Omeprazole	28.95	419.89			
Ondansetron	13.63	57.90	115.80		
Paracetamol	661.54	27.27	81.81		
Penicillamine		1984.62	3307.70	5.12	(Ogungbenro <i>et al.</i> ,
Penicillin		1675.48			
Phenobarbital		713.49			
Phenytoin	64.59		430.60		
	99.10	198.20	396.40		

Additional references: (BNF, 2011; PubChem, 2011; WHO, 2011)

Table 8.10. Dose levels and observed absorption rate constants (k_a) of drugs included in the 17th WHO model list of Essential Medicines.

Drugs	Low dose (μmoles)*	Medium dose (μmoles)*	High dose (μmoles)*	k_a (h^{-1})	References
Praziquantel	480.14		1920.58		
Prednisolone	13.87		69.36		
Primaquine	28.92		57.84		
Proguanil		394.12		0.51	(Hussein <i>et al.</i> , 1996)
Propranolol	77.12		154.24	0.97	(Parsons <i>et al.</i> , 1976)
Propylthiouracil		293.72		1.44	(Kampmann <i>et al.</i> , 1998)
Pyrantel		1211.78			
Pyrazinamide	1218.40	3249.06	4061.32	2.58	(Peloquin <i>et al.</i> , 1997)
Pyridostigmine		229.78		0.32	(Marino <i>et al.</i> , 1998)
Pyridoxine		147.77			
Pyrimethamine		100.52		1.31	(Trenque <i>et al.</i> , 2004)
Quinine		924.74		0.68	(Supanaranond <i>et al.</i> , 2006)
Ranitidine		477.09		1.31	(Hawwa <i>et al.</i> , 2012)
Ribavirin	818.99	1637.97	2456.96	1.45	(Wade <i>et al.</i> , 2006)
Rifabutin		177.09		0.20	(Gatti <i>et al.</i> , 1998)
Rifampicin	182.27		364.55	0.72	(Peloquin <i>et al.</i> , 1997)
Ritonavir	46.19	34.68	69.35	0.18	(Dickinson <i>et al.</i> , 2011)
Saquinavir	298.13		745.33	0.58	(Lavielle and Mentre, 2011)
Simvastatin	11.95	35.84	95.56	2.00	(Gertz <i>et al.</i> , 2011)
Senna		8.69			

Additional references: (BNF, 2011; PubChem, 2011; WHO, 2011)

Table 8.10. Dose levels and observed absorption rate constants (k_a) of drugs included in the 17th WHO model list of Essential Medicines.

Drugs	Low dose (μmoles)*	Medium dose (μmoles)*	High dose (μmoles)*	k_a (h^{-1})	References
Spirinolactone		60.01			
Stavudine	66.90	89.20	133.80	0.45	(Panhard <i>et al.</i> , 2007)
Succimer		548.79			
Sulfadiazine		1997.79			
Sulfamethoxazole	394.82	1579.29	3158.59	2.61	(Li <i>et al.</i> , 2009)
Sulfasalazine		1255.04			
Tenofovir		853.03		1.06	(Baheti <i>et al.</i> , 2011)
Thioguanine		239.25			
Triclabendazole		695.10			
Trimethoprim	68.89	275.56	551.12	1.60	(Jelliffe <i>et al.</i> , 1997)
Valproic acid	693.43	1386.85	3467.13	4.10	(Williams <i>et al.</i> , 2002)
Verapamil	87.99		175.98	1.72	(Gupta <i>et al.</i> , 2002)
Warfarin	1.62	4.86	16.22	1.66	(Lane <i>et al.</i> , 2011)
Zidovudine	224.52	654.84	1122.58	2.86	(Panhard <i>et al.</i> , 2007)
Zinc sulphate		123.88			

Additional references: (BNF, 2011; PubChem, 2011; WHO, 2011)

8.5.2 Mechanism-based inhibitor parameters

Table 8.11. Mechanism-based inhibitors with corresponding inhibitory parameters based on review by Zhou, and co-workers, 2005.

Drug	LogP _{o:w}	LogD _{o:w}	C _{mic} (mg/mL)	f _{u,mic}	K _{I,u} (μM)	k _{inact} (h ⁻¹)	References
Fluoxetine	3.798	3.76	0.1	0.99	5.19	1.02	(Mayhew <i>et al.</i> , 2000)
K11002	3.896	3.896	0.2	0.97	0.49	1.56	(Jacobsen <i>et al.</i> , 2000)
N-desmethyl diltiazem	3.866	1.7	0.1	0.93	0.72	1.62	(Mayhew <i>et al.</i> , 2000)
17α- ethynylestradiol	4.106	4.11	0.1	0.99	17.75	2.40	(Lin <i>et al.</i> , 2002)
Dihydralazine	0.739	0.74	0.25	0.97	33.81	3.00	(Masubuchi and Horie, 1999)
Tamoxifen	5.133	3.45	0.05	0.99	0.20	3.06	(Zhao <i>et al.</i> , 2002)
K11777	3.962	3.81	0.2	0.97	0.06	3.24	(Jacobsen <i>et al.</i> , 2000)
Irinotecan	3.726	1.7	0.1	0.94	22.52	3.60	(Zhou <i>et al.</i> , 2005)
Silybin	4.232	3.97	0.1	0.98	31.52	3.60	(Sridar <i>et al.</i> , 2004)
Clarithromycin	2.805	1.71	0.1	0.97	5.32	4.32	(Mayhew <i>et al.</i> , 2000)
Amprenavir	2.678	2.68	0.1	0.99	1.38	4.38	(von Moltke <i>et al.</i> , 2000)
Ritonavir	2.333	2.33	1.025	0.87	0.06	4.68	(Koudriakova <i>et al.</i> , 1998)
N-desmethyl- tamoxifen	5.149	2.84	0.05	0.98	2.55	4.80	(Zhao <i>et al.</i> , 2002)
Tabimorelin	4.043	1.71	0.1	0.92	4.34	4.80	(Zdravkovic <i>et al.</i> , 2003)
Erythromycin	1.909	0.81	0.1	0.92	43.10	4.80	(Zhou <i>et al.</i> , 2005)
Isoniazid	-0.766	-0.77	0.1	0.99	224.8	4.80	(Wen <i>et al.</i> , 2002)
Mifepristone	6.193	6.18	0.1	0.99	5	5.34	(He <i>et al.</i> , 1999)
Verapamil	4.024	2.08	0.5	0.81	4.63	5.40	(Yeo and Yeo, 2001)
Oleuropein	-0.865	-0.87	0.1	0.99	1.38	5.40	(Zhou <i>et al.</i> , 2005)
SN-38	1.895	1.87	0.1	0.99	21.89	6.00	(Zhou <i>et al.</i> , 2005)

References: (Zhou *et al.*, 2005)

LogP_{o:w}=Octanol-water partition coefficient, LogD_{o:w}=Octanol-water distribution coefficient,

C_{mic}=Concentration of microsomes in assay, f_{u,mic}=fraction unbound

Inhibitor in microsomal assay, K_{I,u}=Inhibitor concentration producing half of the maximal rate of inactivation, k_{inact}=Maximal rate of enzyme inactivation.

Table 8.11. (Continued) Mechanism-based inhibitors with corresponding inhibitory parameters based on review by Zhou, and co-workers, 2005.

Drug	LogP _{o:w}	LogD _{o:w}	C _{mic} (mg/mL)	f _{u,mic}	K _{i,u} (μM)	k _{inact} (h ⁻¹)	References
Diltiazem	4.727	2.98	0.075	0.98	1.96	6.60	(Jones <i>et al.</i> , 1999)
Glabridin	4.105	4.1	0.1	0.99	6.90	8.40	(Kent <i>et al.</i> , 2002)
Troleandomycin	3.46	2.56	0.1	0.98	0.18	9.00	(Zhou <i>et al.</i> , 2005)
Midazolam	3.798	3.76	0.1	0.99	5.72	9.00	(Khan <i>et al.</i> , 2002)
Raloxifene	4.569	3.05	0.1	0.97	9.64	9.60	(Chen <i>et al.</i> , 2002)
6',7'-dihydroxy- bergamottin	2.261	2.26	0.5	0.93	55.11	9.60	(Schmiedlin-Ren <i>et al.</i> , 1997)
Nelfinavir	7.278	7.25	1	0.88	4.90	10.80	(Lillibridge <i>et al.</i> , 1998)
Resveratrol	3.024	3.02	1	0.88	17.52	12.00	(Chan and Delucchi, 2000)
DPC 681	4.856	4.57	0.01	1.00	0.24	13.20	(Luo <i>et al.</i> , 2003)
(-)-Hydrastine	2.458	2.28	0.5	0.93	102.0 3 1068.	13.80	(Chatterjee and Franklin, 2003)
Diclofenac	4.548	1.77	0.5	0.65	81	14.76	(Masubuchi <i>et al.</i> , 2002)
Bergamottin	5.382	5.38	0.5	0.93	3.92	18.00	(Schmiedlin-Ren <i>et al.</i> , 1997)
Mibefradil	6.213	3.9	0.1	0.97	2.23	24.00	(Prueksaritanont <i>et al.</i> , 1999)
Gestodene	2.022	2.02	0.1	0.99	45.36	24.00	(Guengerich, 1990)
Delavirdine	3.534	1.48	0.75	0.61	5.81	26.40	(Voorman <i>et al.</i> , 1998)
L-754,394	4.105	3.87	0.1	0.98	7.39	97.20 120.0	(Lightning <i>et al.</i> , 2000)
Nicardipine	4.893	4.41	1	0.86	0.52	0	(Ma <i>et al.</i> , 2000)

References: (Zhou *et al.*, 2005)

LogP_{o:w}=Octanol-water partition coefficient, LogD_{o:w}=Octanol-water distribution coefficient,
C_{mic}=Concentration of microsomes in assay, f_{u,mic}=fraction unbound Inhibitor in microsomal assay,
K_{i,u}=Inhibitor concentration producing half of the maximal rate of inactivation, k_{inact}=Maximal rate of
enzyme inactivation.

8.5.3 *Nested enzyme-within-enterocyte model code*

The following script was developed by Adam S. Darwich, University of Manchester. Code optimisation was carried out with the assistance of Mr. Mike Croucher, University of Manchester.

Run file

```
%% NEWE model: Developed by Adam Darwich, University of
% Manchester
clear
%% MAIN INPUT PARAMS
dose_i=100000; % umol
n_cells=10;
cell_cycles=5*n_cells;

%% PARAMS
dlmwrite('n_cells_b.txt',n_cells,'delimiter','D');
cellzero=0+(1-0).*rand(1,n_cells);
dose_i_sim=dose_i;
m=0;
a_cyp3a_gi=(90.8*(10^(-3)));
% nmol/total gut -> umol/total gut
a_cyp3a_gi_zero=repmat(a_cyp3a_gi,1,n_cells);
mppgl=39.7907;
% mg protein/g liver
v_hep=1.591; % L
d_hep=1080; % g/L
a_cyp3a_hep=240*mppgl*v_hep*d_hep*(10^(-6));
% pmol/mg protein -> umol/liver
ycell=zeros(2000,n_cells);
tcell=zeros(2000,n_cells);
ycycle=zeros(2000,n_cells);
tcycle=zeros(2000,n_cells);

%% ODE-SOLVER
```

```

tstart = 0;
tfinal = 200;
yzero=[ cellzero'; a_cyp3a_gi_zero'; dose_i_sim;
zeros(2,1); a_cyp3a_hep; zeros(4,1)];

refine = 4;
options=odeset('Events',@a_cyp3a_MBI_eventfun_B,...
'Refine',refine);
tout = tstart;
yout = yzero.';
teout = [];
yeout = [];
ieout = [];

tic
    for i = 1:cell_cycles
        [t y te ye
ie]=ode15s(@a_cyp3a_MBI_model_INHIB_ONLY_B,(tstart:0.01:tfi
nal),yzero,options);
        % Accumulate output: cell,intra.
        nt = length(t);
        tout = [tout; t(2:nt)];
        yout = [yout; y(2:nt,:)];
        teout = [teout; te];
        yeout = [yeout; ye];

        [num idx] = max(t(:));

        % Set new inicon.
        for i = 1:n_cells
            if y(idx,i) >= 1
                yzero(i) = 0;
                yzero(i+n_cells) = a_cyp3a_gi;
            elseif y(idx,i) < 1
                yzero(i) = y(idx,i);

```

```

        yzero(i+n_cells) = y(idx,i+n_cells);
    end
end

yzero(1+n_cells*2) = y(idx,1+n_cells*2);
yzero(2+n_cells*2) = y(idx,2+n_cells*2);
yzero(3+n_cells*2) = y(idx,3+n_cells*2);
yzero(4+n_cells*2) = y(idx,4+n_cells*2);
yzero(5+n_cells*2) = y(idx,5+n_cells*2);
yzero(6+n_cells*2) = y(idx,6+n_cells*2);
yzero(7+n_cells*2) = y(idx,7+n_cells*2);
yzero(8+n_cells*2) = y(idx,8+n_cells*2);

tstart = t(nt);
end
toc

```

Model

```

%% FUNCTION: A_Enterocyte,CYP3A
function dY=a_cyp3a_MBI_model_INHIB_ONLY_B(t,y,te,ye,ie)

%% MODELPARAM
n_cells=load('n_cells_b.txt');
dY=zeros(8+n_cells*2,1);

%% PHYSPARAM
bw=75; % kg
v_sit=(126+44+31+24+18+12)/1000; % L
v_ent=0.517;
v_pv=0.07;
v_hep=1.591;

d_hep=1080; % g/L

q_villi=19; % L/h

```

```

q_pv=74.1;
q_ha=23.35;

k_sit=0.21; % 1/h

kdeg_ent=0.042;
kdeg_hep=0.02;
kdeg_cyp3a=0.001; % 1/h

mppgl=39.7907;
% mg microsomal protein/g liver

mppi=2978;
% mg microsomal protein/total gut

a_cyp3a_gi=90.8*(10^(-3));
% nmolP450/total gut -> umolP450/total gut

a_cyp3a_hep=240*mppgl*v_hep*d_hep*(10^(-6));
% pmolP450/mg protein -> umolP450/liver

%% DRUGPARAM1 (Inhibitor)
ka_i=10;
clu_intl_i=0.01*60*10^(-6);
% uL/min/mg microsomal protein -> L/h/mg microsomal protein
k_inact_3a_i=2000;
% 1/h

k_i_i=2;
% umol/L

fu_i=0.25;
bp_i=0.96;

```

```

fu_b_i=fu_i/bp_i;
fu_gut_i=1;

v_i=1*bw - 3.6*v_hep*(d_hep/1000);
% L/kg -> L

% Inhibitor
clu_intl_gut_i=clu_intl_i*mppi;
clu_intl_hep_i=clu_intl_i*mppgl*v_hep*d_hep;

%% ODE MODEL
%% Inhibitor:
for a = 1:n_cells

    dY(a)=0 + kdeg_ent;

    % y(2; n_cells:n_cells*2)-Enterocytes: Inhib.
    dY(a+n_cells)=(a_cyp3a_gi)*kdeg_cyp3a - ...
    kdeg_cyp3a*y(a+n_cells) - y(a+n_cells)* ...
    (((k_inact_3a_i*fu_gut_i*y(2+n_cells*2))/ ...
    (k_i_i+fu_gut_i*y(2+n_cells*2)))) );
end

% A_CYP3A-GIT: Mean and sum
x_a_cyp3a_gi=mean(y((n_cells+1):(n_cells*2)));
% x_a_cyp3a_gi=sum(y(1:n_cells));

% y(3)-Inhib: Conc_(gut lumen).
dY(1+n_cells*2)=-y(1+n_cells*2)*(ka_i + k_sit);

% y(4)-Inhib: Conc_ent.
dY(2+n_cells*2)=(y(1+n_cells*2)*ka_i -
y(2+n_cells*2)*q_villi -
clu_intl_gut_i*fu_gut_i*y(2+n_cells*2))/v_ent;

```

```

% y(5)-Inhib: Conc_pv.
dY(3+n_cells*2)=(y(2+n_cells*2)*q_villi +
y(7+n_cells*2)*q_pv - y(3+n_cells*2)*q_pv)/v_pv;

% y(6)-Hepatocytes: Inhib.
dY(4+n_cells*2)=a_cyp3a_hep*( kdeg_hep + kdeg_cyp3a ) -
y(4+n_cells*2)*((kdeg_hep + kdeg_cyp3a) +
((k_inact_3a_i*fu_b_i*y(6+n_cells*2))/(k_i_i+fu_b_i*y(6+n_c
ells*2)))));

% y(7)-Hepatocytes: Cell cycle.
dY(5+n_cells*2)=0;

% y(8)-Inhib: Conc_hep.
dY(6+n_cells*2)=(y(3+n_cells*2)*q_pv + y(7+n_cells*2)...
*q_ha - y(6+n_cells*2)*(q_pv + q_ha)...
- clu_int1_hep_i*fu_b_i*y(6+n_cells*2))/v_hep;

% y(9)-Inhib: Conc_sys.
dY(7+n_cells*2)=(y(6+n_cells*2)*(q_pv + q_ha)...
- y(7+n_cells*2)*(q_pv + q_ha))/v_i;

% y(10)-Inhib: Conc_RoB.
dY(8+n_cells*2)=0;

```

Mex function in C++ programming language

```
#include<mex.h>

void mexFunction( int nlhs, mxArray *plhs[], int
nrhs, const mxArray *prhs[]) {

    double *n_cellsP;
    double *DYP;
    double *a_cyp3a_giP;
    double *kdeg_cyp3aP;
    double *yP;
    double *k_inact_3a_iP;
    double *fu_gut_iP;
    double *k_i_iP;
    double *kdeg_entP;
    int a, n_cells;
    double temp_prod1,temp_prod2;

    /* create pointers to the inputs */
    n_cellsP = mxGetPr(prhs[0]);
    DYP = mxGetPr(prhs[1]);
    a_cyp3a_giP = mxGetPr(prhs[2]);
    kdeg_cyp3aP = mxGetPr(prhs[3]);
    yP = mxGetPr(prhs[4]);
    k_inact_3a_iP =mxGetPr(prhs[5]);
    fu_gut_iP = mxGetPr(prhs[6]);
    k_i_iP = mxGetPr(prhs[7]);
    kdeg_entP = mxGetPr(prhs[8]);

    n_cells= (int) n_cellsP[0];
```

```

        temp_prod1 = a_cyp3a_giP[0]*kdeg_cyp3aP[0];
/*in the original, this was calculated every
loop iteration despite the fact that they are
constants.*/
        temp_prod2 = k_inact_3a_iP[0]*fu_gut_iP[0];
        for (a=0; a<n_cells; a++){

                DYP[a] = kdeg_entP[0];
                DYP[a+n_cells]= temp_prod1 -
kdeg_cyp3aP[0]*yP[a+n_cells] -
yP[a+n_cells]*(((temp_prod2*yP[1+n_cells*2]))/(k_i
_iP[0]+fu_gut_iP[0]*yP[1+n_cells*2]))) );

        }
}

```

Event function

```

function [value,isterminal,direction] =
a_cyp3a_MBI_eventfun_B(t,y)

% Param
n_cells=load('n_cells_b.txt');
cell_v=1:1:n_cells;
value = y(cell_v') - 1; % value = 1, event is triggered
isterminal(1:n_cells') = 1; % terminate after the first
event
direction = 0; % get all the matrix of zeros

```


8.5.4 References

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8.6 Discussion and conclusions

8.6.1 Midazolam following Roux-en-Y gastric bypass

The compound file for midazolam in Simcyp Simulator was adapted for immediate release formulation using the ADAM model (Table 8.12) (Turner, 2008; Jamei *et al.*, 2009).

Table 8.12. Simcyp Simulator midazolam compound file parameters.

Parameters	Value	References
PhysChem		
MW (g/mol)	325.8	(Turner, 2008; NCBI, 2011)
LogP _{o:w}	3.53	
Acid-base nature	Ampholyte	
pKa	10.95, 6.2	
Blood binding		
BP	0.603	(Turner, 2008)
fu _p	0.035	
Dissolution		
Solubility method	Intrinsic solubility estimation toolbox	(Turner, 2008)
Solubility (mg/mL)	0.015	
Particle Size (um)	10	
Supersaturation ratio	4	
Absorption		
P _{eff,man}	6.045	(Turner, 2008)
Distribution		
V _{ss} (L/kg)	1	(Turner, 2008)
Distribution model	Minimal PBPK	
Metabolism		
CYP3A4: 1-OH		(Turner, 2008)
V _{max} (pmol/min/pmol P450)	5.23	
K _m (μM)	2.16	
CYP3A4: 4-OH		
V _{max} (pmol/min/pmol P450)	5.2	
K _m (μM)	31.8	
CYP3A5: 1-OH		
V _{max} (pmol/min/pmol P450)	19.7	
K _m (μM)	4.16	
CYP3A5: 4-OH		
V _{max} (pmol/min/pmol P450)	4.03	
K _m (μM)	34.8	
Additional clearance		
CL _R (L/h)	0.085	

BP =Blood to plasma ratio, fu_p=fraction unbound in plasma, P_{eff,man}=effective human jejunal permeability, V_{ss}=Volume of distribution at steady state following intravenous infusion.

Midazolam IR using the ADAM model was validated against a semisimultaneous p.o. dose of 5 mg followed by a 2 mg intravenous infusion over 30 minutes at 6 hours post oral dosing in healthy volunteers (n=12) weighing 66.1 ± 15.2 kg and aged between 19 and 42 years (Lee *et al.*, 2002). Performance was evaluated using visual predictive check (Figure 8.5).

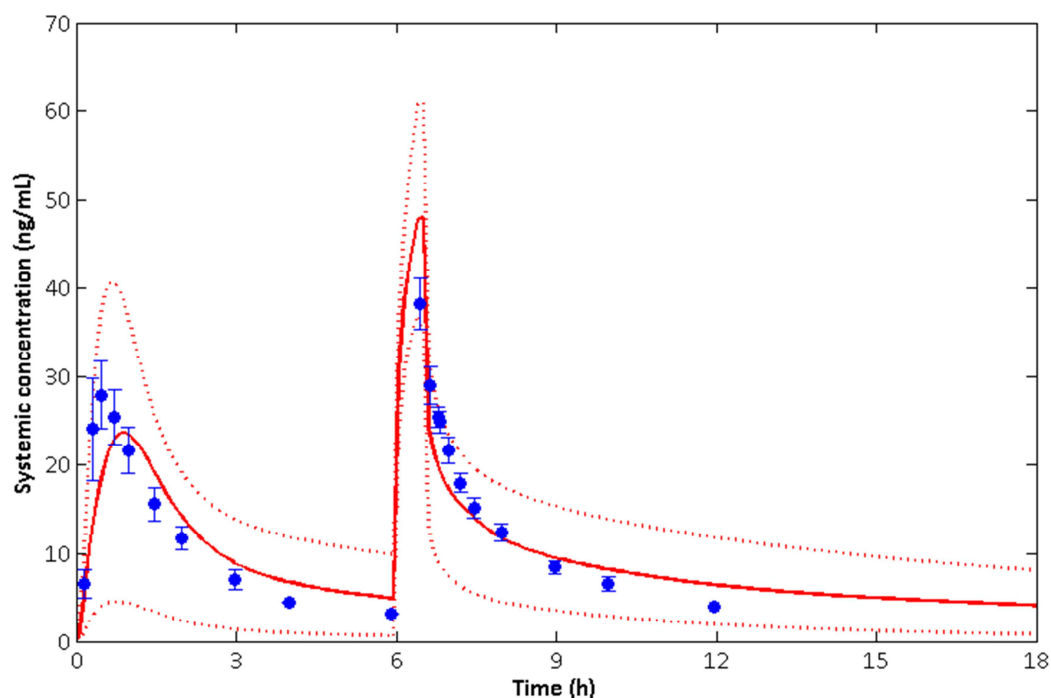


Figure 8.5. Simulated midazolam in healthy volunteers administered as an immediate-release 5 mg oral dose using the Advanced Dissolution Absorption and Metabolism (ADAM) model followed by a 30 minute intravenous infusion of 2 mg midazolam 6 hours post oral dosing as compared to observed data in 12 individuals. Observed data digitised using GetData Graph Digitiser (Lee *et al.*, 2002).

Midazolam IR 7.5 mg followed by an intravenous bolus of 5 mg at 150 minutes after the oral dose was simulated in morbidly obese pre to post Roux-en-Y gastric bypass utilising developed models (Darwich *et al.*, 2012). Oral midazolam displayed a 1.13-fold increase in exposure following Roux-en-Y gastric bypass (small intestinal transit=2.5h) mainly due to an increase in F_G (Figure 8.6).

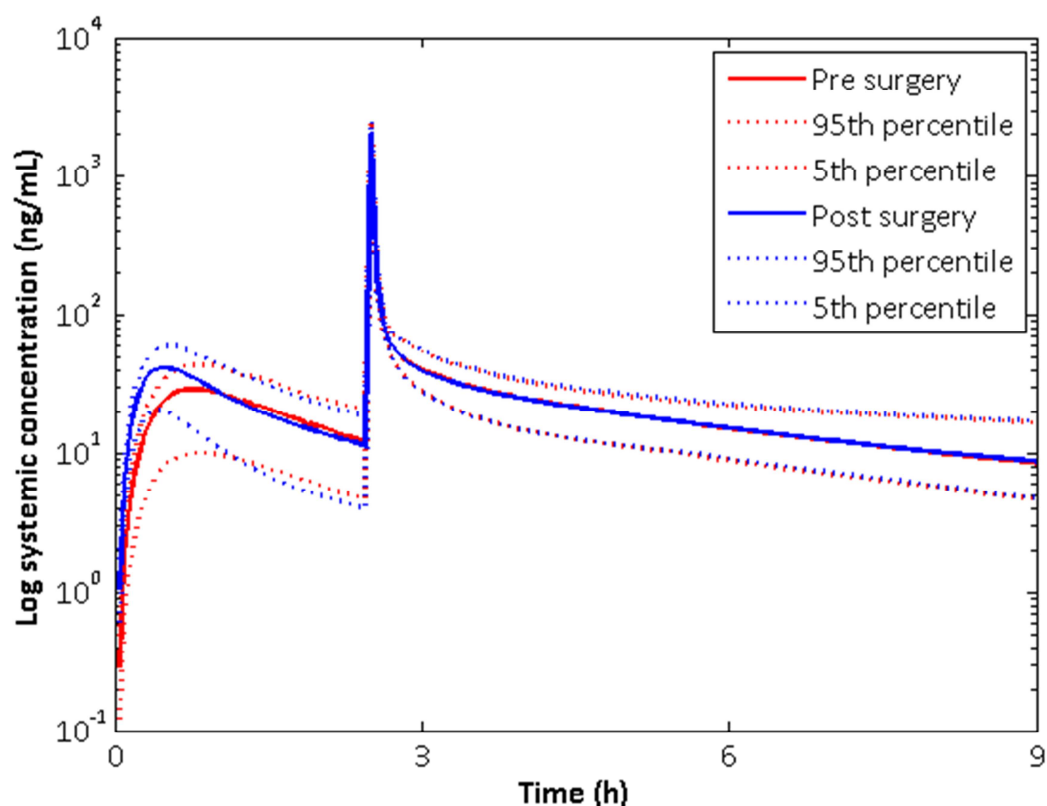


Figure 8.6. Simulated midazolam pre to post Roux-en-Y gastric bypass in morbidly obese administered as an immediate-release 7.5 mg followed by a 30 minute infusion of 5 mg over 150 minutes post oral dosing.

8.6.2 References

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