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## Non-invasive biophysical measurement of travelling waves in the insect inner ear

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6 2 **Non-invasive biophysical measurement of travelling waves in the insect inner ear**

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**Abstract**

Frequency analysis in the mammalian cochlea depends on the propagation of frequency information in the form of a travelling wave (TW) across tonotopically arranged auditory sensilla. TWs have been directly observed in the basilar papilla of birds and the ears of bush-crickets (Insecta: Orthoptera) and have also been indirectly inferred in the hearing organs of some reptiles and frogs. Existing experimental approaches to measure TW function in tetrapods and bush-crickets are inherently invasive, compromising the fine-scale mechanics of each system. Located in the forelegs, the bush-cricket ear exhibits outer, middle and inner components; the inner ear containing tonotopically arranged auditory sensilla within a fluid-filled cavity, and externally protected by the leg cuticle. Here, we report bush-crickets with transparent ear cuticles as potential model species for direct, non-invasive measuring of TWs and tonotopy. Using laser Doppler vibrometry and spectroscopy, we show that increased transmittance of light through the ear cuticle allows for effective non-invasive measurements of TWs and frequency mapping. More transparent cuticles allow several properties of TWs to be precisely recovered and measured in vivo from intact specimens. Our approach provides an innovative, non-invasive alternative to measure the natural motion of the sensillia-bearing surface embedded in the intact inner ear fluid.

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## 1. Introduction

Among vertebrates, mammals and birds exhibit an elaborate hearing system, in which auditory perception relies on mechanical and neurophysiological processes occurring in the fluid-filled cochlea [1]. Frequency discrimination occurs in the cochlea, a coiled, fluid filled structure of bone located inside the skull. Sound is decomposed in a spatial frequency map characterised as tonotopy. This is supported by an oscillatory motion travelling along the length of the basilar membrane, a structure inside the cochlea, which bears the stereocilia (sensory cells). This travelling wave (TW) propagates inside the cochlea and generates an amplitude maxima response at frequency-dependent locations [2]. The mechanical displacement at resonant points stimulates the sensory receptor cells initiating a neural response.

First used to describe the motion of the basilar membrane in the cochleae of human cadavers [3], passive TWs are viewed today as the substratum for active cochlear amplification in mammals [1, 4]. Phenomena analogous to TW have been directly observed in the basilar papilla of birds (Aves) [5] and the ears of bush-crickets (Insecta) [6, 7], and have also been inferred, via the timing of responses of auditory-nerve fibres, in the hearing organs of some reptiles and frogs [8, 9]. In vertebrates, the structure and location of the inner ear make it almost impossible to access without altering its integrity [1, 7, 10].

Measurements *in vivo* have only been done through small openings in the *scala tympani* or other isolated places [10, 11, 12]. Indirectly, the spatial frequency response on the basilar membrane (BM) has also been inferred through computational models, or estimated from auditory afferent nerve fibres at selected points [13, 14]. Hitherto, there lacks an easy, non-invasive approach to directly access the complex auditory processes occurring with the cochlea

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4 62 Bush-crickets (Orthoptera: Tettigoniidae) are insects that exploit acoustic signals to interact  
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6 63 with their conspecifics [15-17]. Both males and females detect acoustic signals using paired  
7  
8 64 tympanal organs located on their forelegs (figure 1a), just below the femoro-tibial joint [18-  
9  
10 65 20]. The tympanal organ is backed by an acoustic tracheal tube connecting the ear with the  
11  
12 66 thoracic spiracle [21]. Just at the tympanal region the trachea splits in two forming a fold with  
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14 67 a triangular and slightly curved/convex surface, which contains a collection of  
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16 68 mechanoreceptors aligned in a row forming a crest, known as the *crista acustica* (CA).  
17  
18 69 Bush-crickets exhibit a highly-sophisticated hearing system that includes an outer, middle,  
19  
20 70 and an inner ear, which exhibit basic auditory processes analogous to the mammalian  
21  
22 71 system [6]. Although a large number of questions remain to be answered before the two  
23  
24 72 ears can be seen as equivalent, both systems can be compared in a broad sense. The  
25  
26 73 bush-cricket inner ear formed by the CA and auditory vesicle (AV), allows effective  
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28 74 frequency discrimination through tonotopy and TWs [22-24]. Similar to the mammalian  
29  
30 75 basilar membrane in the cochlea, sound-induced TWs originate at the narrow, distal, high-  
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32 76 frequency end of the CA, and propagate towards the wide, low-frequency, proximal region of  
33  
34 77 the same structure [6, 7]. This mechanical motion enhances the tonotopic response at a  
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36 78 specific resonant location where the TW reaches its maximum displacement [25].  
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40 80 Innovative approaches and organisms with easy-to-access inner ears could provide  
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42 81 alternative solutions to advance our understanding of complex auditory processes. Bush-  
43  
44 82 crickets provide an ideal model, having ears which lays beneath the leg cuticle allowing  
45  
46 83 researchers to measure TWs and tonotopy by removing the leg cuticle and exposing the  
47  
48 84 organs of the inner ear [7, 26]. This current available method has also been used with  
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50 85 electrophysiology to measure the responses of sensory cells to sound-induced mechanical  
51  
52 86 forces [25]. Yet this protocol might have negative effects in the natural operation of the ear.  
53  
54 87 For example, draining the AV's fluid compromises the hydrostatic equilibrium of the system  
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56 88 [6, 27]. On the other hand, some auditory processes in the inner ear of bush-crickets were  
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4 89 measured non-invasively using laser Doppler vibrometry (LDV) [6]. The authors speculated  
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6 90 that this possible perhaps due to either translucent or thin ear cuticles, yet the mechanism  
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8 91 by which this was possible is not understood [27]. Thus, understanding the properties of the  
9  
10 92 ear cuticle is of fundamental importance for furthering research on measuring auditory  
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12 93 activity using non-invasive techniques.

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15  
16 95 In this study, we quantified cuticle transparency across six species with different levels of  
17  
18 96 cuticular pigmentation, and established the relationship between transparency, cuticle  
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20 97 thickness, and LDV measurements of auditory activity. We hypothesise that transparency is  
21  
22 98 the main cuticle property allowing the precise recording, and measurement of TWs and  
23  
24 99 tonotopy in the inner ear of bush-crickets. Using the species with the highest cuticular  
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26 100 transparency, the glass bush-cricket *Phlugis poecila*, we exemplify the retrieval of these  
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28 101 complex auditory parameters from the inner ear, achieved non-invasively *in vivo*.

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## 32 33 103 **2. Materials and Methods**

### 34 35 36 104 **2.1. Specimens**

37  
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39 105 Female and male adults of *Copiphora gorgonensis*, *C. vigorosa*, *Phlugis poecila*,  
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41 106 *Neoconocephalus affinis*, *Nastonotus foreli*, and *Acantheremus* sp. were taken from  
42  
43 107 colonies reared at the University of Lincoln, UK. Parental specimens were initially collected  
44  
45 108 from two locations in the Colombian rain forest during December 2014 and November 2015.  
46  
47 109 Collecting events took place at night (18:00 – 24:00) along established trails in the sampling  
48  
49 110 areas, with a total of 48 hours of sampling activity. The sampling locations were El palmar de  
50  
51 111 la Vizcaína and the National Natural Park, Gorgona. The former is an oil palm research  
52  
53 112 centre surrounded by patches of tropical rain forest situated in the valley of the Magdalena  
54  
55 113 river, 32 km from the municipality of Barrancabermeja, Santander (lat. 6°59'02.3"N; long  
56  
57 114 73°42'20.2"W). The latter is an island situated at 35 km from the Pacific coast of Colombia  
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4 115 (lat 2°47' to 3°6' N; long 78°6', to 78°18'W). The park's ecosystem is classified as tropical  
5  
6 116 wet forest with an area of 13.33 km<sup>2</sup>. Collected specimens were transported to the University  
7  
8 117 of Lincoln, UK, under collection and exportation permit No COR 5494-14 (issued by the  
9  
10 118 Administrative Unit of National Natural Parks of Colombia).

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## 14 15 120 **2.2. Cuticle transparency measurements**

16  
17  
18 121 Cuticle transparency was quantified by measuring the transmittance (ratio of the transmitted  
19  
20 122 radiant flux to the incident radiant flux) of the cuticle covering the hearing organ. Cuticle  
21  
22 123 samples were dissected from live specimens and placed in a cavity well microscope slide  
23  
24 124 containing insect saline solution [28]. A 50 µm diameter optic fibre connected to a  
25  
26 125 spectrophotometer (USB2000 Fibre Optic Spectrometer, Ocean optics Inc., Oxford, UK) was  
27  
28 126 placed on the projector lens in the camera ocular of a compound light microscope. For all  
29  
30 127 the measurements a 40X objective lens was used and the reference light was the  
31  
32 128 illumination system of the microscope (Halogen lamp), with brightness maintained at 5 volts  
33  
34 129 consistently for all experiments. The spectrophotometer detector unit was connected to a  
35  
36 130 computer via an USB port and the collected measurements were transformed into digital  
37  
38 131 format using the OOIBase32 spectrophotometer operating software (Ocean Optics Inc.,  
39  
40 132 Oxford, UK). The software calculates the percentage of energy passing through a sample  
41  
42 133 relative to the amount that passes through the reference (equation 1).

43  
44  
45 134 
$$\%T_{\lambda} = \frac{S_{\lambda} - D_{\lambda}}{R_{\lambda} - D_{\lambda}} \times 100\% \quad (1)$$

46  
47  
48 135 Where %T<sub>λ</sub> is the percentage of transmittance at wavelength λ, S<sub>λ</sub> is the sample intensity, D<sub>λ</sub>  
49  
50 136 is the dark intensity, R<sub>λ</sub> is the reference intensity [29].

51  
52  
53 137 For each transmittance measurement a reference spectrum was taken with the light source  
54  
55 138 on and a blank in the sampling region. The dark reference spectrum was taken with the light

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4 139 path blocked, and a stray light correction was applied using boxcar pixel smoothing and  
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6 140 signal averaging (10 averages).

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11 142 **2.3. Artificial actuator vibrations measured through transparent cuticle**

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13  
14 143 A piece of freshly dissected cuticle from the dorsal ear area and a reference vibratory  
15  
16 144 surface were used to evaluate the effects of the cuticle transparency on the laser Doppler  
17  
18 145 vibrometry measurements, and to investigate whether the laser records ear vibrations on the  
19  
20 146 cuticle, or on the CA through the cuticle. Ear top cuticles were dissected from one of the  
21  
22 147 forelegs of live specimens from all species excluding *N. affinis* and fixed with a mixture of  
23  
24 148 beeswax (Fisher Scientific, Bishop Meadow Road, Loughborough, UK) and colophonium  
25  
26 149 (Sigma-Aldrich, Dorset, UK) to the tip of a copper rod (0.632 cm diameter and 23 cm long).  
27  
28 150 Using a micromanipulator the external surface of sample was placed perpendicular between  
29  
30 151 the laser head and the cone of a tweeter speaker enclosed in a custom made acoustic  
31  
32 152 attenuating box (figure 2a). A 30 kHz pure tone was used as a reference signal and a 1/8"  
33  
34 153 condenser microphone (Brüel & Kjaer, 4138-A-015 and preamplifier model 2670, Brüel &  
35  
36 154 Kjaer, Nærum, Denmark) was positioned approximately 2-3 mm from the cuticle to monitor  
37  
38 155 the acoustic isolation of the attenuating box and to ensure that the sound stimulus was not  
39  
40 156 eliciting vibrations on the cuticle. The laser beam was focused on the cuticle and a digital  
41  
42 157 scanning grid of approximately 450 points was set on the dorsal surface of the piece of  
43  
44 158 cuticle. The recording time for each of the measuring points was 32 ms (5 averages), with a  
45  
46 159 sampling rate of 512 kHz. The vibratory response was measured in displacement after  
47  
48 160 applying a 1 kHz high-pass filter. As a control, the cuticle was removed and the surface of  
49  
50 161 the speaker was scanned using the same settings and grid of points. The effect of the cuticle  
51  
52 162 on the laser signal was estimated by calculating the ratio between the displacement  
53  
54 163 response of the laser beam through the cuticle and the control surface.

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#### 165 **2.4. Cuticle thickness**

166 Cuticle thickness was measured to evaluate the effects of this property on the laser signal  
167 response. For this, the previously dissected cuticle samples were cut transversally  
168 lengthwise down the midpoint of the sample. Samples were then placed on an aluminium  
169 scanning electron microscope stub using a carbon tape. Digital images were captured and  
170 analysed with a FEI Inspect S50 microscope (FEI, Hillsboro, OR, USA). Measurements were  
171 made with the graphics software Coreldraw X7 (Corel corporation, Ottawa, Canada) using  
172 the dimension tool and adjusting the scale to real world values using the scale bar from each  
173 individual SEM image (electronic supplementary material, figure S1).

174

#### 175 **2.5. Mounting the specimens for LDV measurements of travelling waves**

176 Protocols for measuring ear activity with LDV follows Montealegre-Z *et al.* [6]. For the LDV  
177 experiments, insects were initially anesthetized with a triethylamine-based mix (FlyNap®,  
178 Carolina Biological Supply Company, Burlington, North Carolina, USA) to facilitate the  
179 fastening to a horizontal brass platform (5 mm wide, 1 mm thick and 70 mm long). The  
180 dorsal pronotal area and legs, except for the frontal pair, were fixed to the platform using a  
181 mixture of beeswax (Fisher Scientific, Bishop Meadow Road, Loughborough, UK) and  
182 colophonium (Sigma-Aldrich, Dorset, UK). The front legs were restrained using brass wires,  
183 which allowed positioning of the tibia and femur in a 90 degrees angle. Additionally, the  
184 brass plate was attached to an articulated aluminium rod (150 mm long, 8 mm diameter)  
185 allowing the dorsal surface of the ear to be placed perpendicular to the scanner's laser  
186 beam. All experiments were carried out inside an acoustic booth, IAC Acoustics (Series  
187 120a, internal length 2.40 m, width 1.8 m, and height 1.98 m), at room temperature (24–  
188 26°C) and relative humidity of 32-35%. The acoustic booth provides an internal reduction to  
189 external noise of at least 59 dB at 2 kHz and above (manufacturers information). The  
190 scanning head of the laser and the experimental setup were placed on Melles Griot Optical

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4 191 Table Breadboard, Pneumatic Vibration Isolation (1m x 1m area) (Melles Griot, Rochester,  
5  
6 192 NY).

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9 193 **2.6. LDV measurements of travelling waves**

10  
11 194 The sound-induced vibration pattern of the ear was measured using a micro-scanning laser  
12  
13 195 Doppler vibrometer (Polytec PSV-500; Waldbronn, Germany) fitted with a close up  
14  
15 196 attachment. The mounted specimens were positioned so that the cuticle overlaying the ear  
16  
17 197 was perpendicular to the lens of the laser unit. A loudspeaker was positioned 30 cm,  
18  
19 198 ipsilateral to the specimen to broadcast the sound stimulus (electronic supplementary  
20  
21 199 material, figure S2). Periodic chirps were used as the acoustic stimulus, generated by the  
22  
23 200 Polytec software (PSV 9.0.2), passed to an amplifier (A-400, Pioneer, Kawasaki, Japan),  
24  
25 201 and sent to the loudspeaker (Ultrasonic Dynamic Speaker Vifa, Avisoft Bioacoustics,  
26  
27 202 Glienicke, Germany). The periodic chirps contained frequencies between 5 and 80 kHz, and  
28  
29 203 the stimulus was flattened so all frequencies were represented at 60 dB  $\pm$ 1.5 dB (SPL re 20  
30  
31 204  $\mu$ Pa) at the position of the ear. A 1/8" microphone (Brüel & Kjaer, 4138-A-015 and  
32  
33 205 preamplifier model 2670, Brüel & Kjaer, Nærum, Denmark) was placed at the position of the  
34  
35 206 ear to monitor and record the acoustic stimulus at the position of the ear as a reference  
36  
37 207 (electronic supplementary material, figure S2). The laser system was used in scan mode. A  
38  
39 208 grid of scan points on the dorsal surface of the CA was established using the PSV 9.2  
40  
41 209 acquisition software (Polytec, Waldbronn, Germany). Depending on the size of the insect's  
42  
43 210 leg, the actual number of measuring points per grid varied among specimens, with ~800  
44  
45 211 points per ear. Within the frequency domain setting of the vibrometer, a frequency spectrum  
46  
47 212 was calculated for each point using a FFT with a rectangular window, at a sampling rate of  
48  
49 213 256 kilo samples/second, 64 ms sampling time with a frequency resolution of 15.625 Hz. A  
50  
51 214 high-pass filter of 1 kHz was applied to the both the vibrometer and reference microphone  
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53 215 signals during the scanning process.

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56 216 **2.7. Data analysis**  
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4 217 The relationship between laser response (a ratio), cuticular thickness ( $\mu\text{m}$ ), and cuticular  
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6 218 transmittance (%) were analysed using linear mixed effects (LMMs). Species was fitted as a  
7  
8 219 random effect to account for species-differences in samples sizes. Parameters were logged  
9  
10 220 before analysis. Models with and without interactions terms between cuticular thickness and  
11  
12 221 cuticular transmittance were tested using likelihood ratio tests. The inclusion of the  
13  
14 222 interaction significantly improved the model ( $\chi^2_1=8.54$ ,  $P<0.001$ ). The relationship between  
15  
16 223 cuticular thickness and transmittance was tested with a Pearson's correlation.

17  
18  
19 224 Data from all scanned points were examined using the PSV 9.2 presentation software  
20  
21 225 (Polytec, Waldbronn, Germany). Frequency spectrums, ear displacement animations, and  
22  
23 226 oscillation profiles were produced for selected frequencies within the recorded range.  
24  
25 227 Frequency spectrums of the vibrometry data were normalised to those of the reference  
26  
27 228 signal by computing the transfer function of the two [30]. For the TWs analysis, coordinates  
28  
29 229 and displacement values from points corresponding to a 1 mm profile line set distal to  
30  
31 230 proximal on the measured grid were exported as an ASCII file. The obtained data points  
32  
33 231 were analysed using a custom Matlab code (Matworks Inc., Nauticks, USA), which  
34  
35 232 generates plots of the TWs recorded from the scanned ears. The plots allowed us to  
36  
37 233 visualise and measure the velocity response of each point in the frequency domain. The  
38  
39 234 graphical representation was used to evaluate two of the TWs' criteria: asymmetric envelope  
40  
41 235 and phase lag [30]. Furthermore, TWs' propagation velocity and wavelength were calculated  
42  
43 236 from the phase response using equations 2-4.

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46 237 
$$\delta_t = \frac{\delta_\phi}{2\pi f} \quad (2)$$

47  
48  
49 238 
$$V_{wave} = \frac{\delta_x}{\delta_t} \quad (3)$$

50  
51  
52  
53 239 
$$\lambda = \frac{2\pi\delta_x}{\delta_\phi} \quad (4)$$

1  
2  
3  
4 240 Where  $f$  is wave frequency (Hz),  $\delta_\phi$  is phase difference (rad) between two points at different  
5  
6 241 locations,  $\delta_t$  is the travel time (s),  $\delta_x$  is the distance travelled (m),  $V_{wave}$  is wave velocity and  
7  
8 242  $\lambda$  is wavelength [1, 30]. We then tested the relationship between these parameters and  
9  
10 243 frequency using LMMs. In each model, individual katydid was fitted as a random effect. For  
11  
12 244 all LMMs, degrees of freedom were calculated using Satterthwaite's approximation.  
13  
14 245 Statistical analysis was carried out using the lme4 package [31] run in R version 3.3.1 [32]  
15  
16  
17 246

### 19 247 **3. Results**

#### 22 248 **3.1. Cuticle transmittance**

24 249 We quantified cuticle transparency across six species (figure 1a), and established the  
25  
26 250 relationship between this property, cuticle thickness and LDV measurements of auditory  
27  
28 251 activity. Using a spectrophotometer, cuticle transparency was quantified by measuring the  
29  
30 252 transmittance (ratio of the transmitted radiant flux to the incident radiant flux) of the cuticle  
31  
32 253 covering the hearing organ. Transmittance percentage values for all measured cuticles  
33  
34 254 increased with wavelength in the visible light spectrum, 370-800 nm (figure 1b). At the light  
35  
36 255 spectrum wavelength of the LDV laser (633 nm, Polytec PSV-500; Waldbronn, Germany)  
37  
38 256 the curves can be distinguished into two groups. One group with transmission values  
39  
40 257 relatively high, *P. poecila* and *C. gorgonensis* with averages of  $73.73\% \pm \underline{3.10}$  and  $59.93\% \pm$   
41  
42 258  $\underline{4.15}$  respectively (mean  $\pm$  SE, figure 1c). The second group includes values below 50% and  
43  
44 259 it is formed by *C. vigorosa*, *Acantheremus* sp. *N. affinis*, and *N. foreli* with transmission  
45  
46 260 percentages of  $40.00\% \pm \underline{3.24}$ ,  $34.14 \pm \underline{12.24}$ ,  $33.46\% \pm \underline{2.32}$ , and  $18.82\% \pm \underline{2.64}$   
47  
48 261 respectively (mean  $\pm$  SE).  
49  
50

#### 52 262 **3.2. Laser Doppler vibrometry ratio response**

53  
54  
55 263 The effect of cuticle transparency specifically in relation to transmission of light from a LDV  
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57 264 was calculated as a ratio of the LDV response (measured as displacement) from a reference  
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4 265 vibrating surface (a membrane on a speaker playing a sine wave, figure 2a), and the same  
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6 266 surface as measured through a sample of ear cuticle. The relationship between this LDV  
7  
8 267 response and cuticle transmission, including cuticle thickness, was quantified through linear  
9  
10 268 regression of these variables. Cuticle thickness was obtained by measuring cross sections  
11  
12 269 of dissected ear cuticle (electronic supplementary material, figure S1). A linear mixed effect  
13  
14 270 model found that laser displacement response ratio ( $L_r$ ) was significantly related to the  
15  
16 271 interaction between cuticle thickness and transmittance values (LMM: cuticular thickness x  
17  
18 272 transmittance  $\beta \pm SE = 0.90 \pm 0.31$ ,  $F_{1,18.07} = 8.53$ ,  $P = 0.009$ ; LMM: cuticular thickness  $\beta \pm SE =$   
19  
20 273  $3.52 \pm 1.11$ ,  $F_{1,16.13} = 9.96$ ,  $P = 0.006$ ; LMM: transmittance  $\beta \pm SE = 4.08 \pm 1.30$ ,  $F_{1,18.07} = 9.82$ ,  
21  
22 274  $P = 0.006$ ). Lowest laser displacement response ratio ( $L_r$ ) occurred when both the cuticle was  
23  
24 275 thin and when transmittance was low (figure 2b); the highest laser displacement response  
25  
26 276 ratio ( $L_r$ ) occurred when transmittance was high and cuticles were thinnest (*P. poecila*:  
27  
28 277  $\text{mean} \pm SE = -0.24 \pm 0.07$ ). Transmittance and cuticle thickness were not correlated ( $r_p = -0.09$ ,  
29  
30 278  $P = 0.667$ ).

### 33 279 **3.3. *In vivo* measurement of travelling waves**

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35  
36 280 In order to corroborate the feasibility of transparent species for *in vivo* audition experiments,  
37  
38 281 the auditory activity of specimens of *P. poecila* was investigated as this species presented  
39  
40 282 the highest transmittance values and thinnest cuticles. Non-invasive measurements of  
41  
42 283 tonotopy and TWs *in vivo* were done by directly measuring the sound-induced vibration  
43  
44 284 pattern of the ear using LDV (figure 3a, example of LDV output, figure 3b-c, see also  
45  
46 285 electronic supplementary material, Movie S1). A spatially discrete response was observed  
47  
48 286 for frequencies between ~10 and ~60 kHz from non-invasive measurements along the  
49  
50 287 length of the hearing organ (figure 4a-d). With increasing stimulus frequency, the maximum  
51  
52 288 response shifts towards the distal part of the leg (figure 4a-d) as predicted by the TW model  
53  
54 289 of cochlea function.

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3  
4 290 The measured response in the inner ear satisfies two criteria for the inference of TWs: (i)  
5  
6 291 asymmetric envelope and (ii) phase lag [1]. The magnitude of CA displacement shows an  
7  
8 292 asymmetric envelope around the point of the maximal deflection. This point is also the  
9  
10 293 location where the wave is seen to compress before dying off. TW asymmetry was  
11  
12 294 evaluated as the response gain (mm/ s/ Pa) along a transect line across the CA for different  
13  
14 295 frequencies (figure 4e-g) and it was observed that the position of the maximum displacement  
15  
16 296 of the TW envelope varies with frequency. At 19 kHz the wave is asymmetrical about 720  
17  
18 297  $\mu\text{m}$  along the transect (figure 4e), at 25 kHz the asymmetry occurs around 577  $\mu\text{m}$  (figure  
19  
20 298 4f), and for 47 kHz the same phenomenon is observed approximately at 447  $\mu\text{m}$  (figure 4g).  
21  
22 299 Similarly, the phase response across the CA displays an increasing lag along the transect  
23  
24 300 (figure 4e-g). The lag increases as a function of frequency; for instance, at 19 kHz the phase  
25  
26 301 lag is  $281^\circ$ , while at 47 kHz the lag reaches  $419^\circ$  difference between the initial and final  
27  
28 302 phase angle.

30  
31 303 Velocity and wavelength of propagation are parameters of TW that can be acutely  
32  
33 304 characterised with our approach. The velocity of the TW in the inner ear of *P. poecila*  
34  
35 305 increased from  $6.22 \pm 1.22$  to  $18.55 \pm 3.04$  in a frequency range of 10 kHz to 50 kHz. The  
36  
37 306 wavelength on the other hand decreased from  $0.62 \pm 0.12$  to  $0.37 \pm 0.06$  for the same  
38  
39 307 frequency range. In our measurements, TW's velocity was significantly positively related to  
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41 308 sound frequency (LMM:  $\beta \pm \text{SE} = 0.31 \pm 0.02$ ,  $F_{1,103} = 315.60$ ,  $P < 0.001$ ; figure 4h). Conversely,  
42  
43 309 there was a significant decrease in wavelength size as frequency increased (LMM:  $\beta \pm \text{SE} =$   
44  
45 310  $0.006 \pm 0.001$ ,  $F_{1,103} = 77.48$ ,  $P < 0.001$ ; figure 4i).

#### 48 311 **4. Discussion**

49  
50 312 We have confirmed cuticle transparency and cuticular thickness as primary factors allowing  
51  
52 313 the non-invasive measurement of TWs and auditory mechanisms in the bush-cricket inner  
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54 314 ear. Furthermore, our analysis reveals that transmittance of light through the cuticle is a  
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56 315 reliable indicator of a species' suitability for experiments specifically using LDV. The lack of  
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4 316 correlation between cuticle transmittance and thickness indicates that pigmentation affects  
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6 317 transparency, and in turn, laser measurements. This explains why established model  
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8 318 species in insect hearing research like *Mecopoda elongata* [7] were not suitable in attempts  
9  
10 319 of non-invasive laser measurements [27].  
11  
12 320 From the six species studied, *P. poecila* is a good model for auditory research due to its  
13  
14 321 exceptional cuticle transparency and hearing capabilities. This could also apply to many  
15  
16 322 species of the same subfamily (Meconematinae) within the genus *Phlugis* or related genera,  
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18 323 which are also known as 'glass' or 'crystal bush-crickets' (or katydids). Males *P. poecila*  
19  
20 324 produce calling songs to attract females using a broadband with a main carrier frequency  
21  
22 325 peaking around 50 kHz (electronic supplementary material, figure S4). Our non-invasive  
23  
24 326 approach shows that the ears of this species also incorporates a wide spectrum of  
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26 327 frequencies from the audible to the ultrasonic range (at least 6-70 kHz, Fig. 4), and overlap  
27  
28 328 the hearing ranges of humans and other vertebrates.

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31 329 Several parameters of the auditory process could be measured non-invasively from the inner  
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33 330 ear using LDV. Yet, to which extent some of the values recovered are real is unknown.  
34  
35 331 Scattering of the laser beam at the cuticle (externally and internally) and at the AV might  
36  
37 332 have an effect of the final values measured (for instance mechanical amplification). The  
38  
39 333 presence of a liquid medium between the cuticle and the CA, reduces the laser beam  
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41 334 scattering by providing a refractive index-matching effect [33]. The chemical composition of  
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43 335 the AV fluid remains unknown, but it is likely that its refractive index, as reported for the  
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45 336 haemolymph of other insects [34], is higher than that of the water (at 1.33). Therefore, due to  
46  
47 337 a possible high refractive index, the AV fluid might increase the resolving power between the  
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49 338 cuticle and the CA, as occurs with the use of immersion oils in light microscopy [35]. Finally,  
50  
51 339 we think that the AV's geometry combined with the refractive index of the liquid together  
52  
53 340 have an optical effect analogous to a plano-convex lens. As a consequence, this property  
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55 341 increases the numerical aperture of the laser beam while reducing the characteristic  
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57 342 irradiance loss of a Gaussian beam [36]. While refractive index of the AV fluid was not  
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4 343 measured in this study, future efforts should aim to account for this optical effect and to  
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6 344 correct the LDV values of velocity/displacement accordingly [37, 38].  
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8  
9 345 Taking advantage of the high level of cuticle transparency and wide frequency bandwidth of  
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11 346 auditory perception (electronic supplementary material, figure S3) in *Phlugis* spp., we  
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13 347 corroborated the use of bush-crickets as an alternative system for the non-invasive study of  
14  
15 348 auditory processes. The observed phase lag and asymmetric envelope along the CA (figure  
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17 349 4e-g) allowed us to characterise the auditory response as a TW with displacement maxima  
18  
19 350 at tonotopically specific locations. The obtained TW velocities and wavelengths are shown  
20  
21 351 (figure 4h and 4i). These parameters have been calculated in the bush-cricket *Mecopoda*  
22  
23 352 *elongata* by opening the cuticle and draining the natural AV fluid [12]. The data presented  
24  
25 353 here was collected non-invasively from an intact system, reducing the effects of surgically  
26  
27 354 opening the inner ear cavity (e.g. changes in the hydrostatic pressures and fluid density [6,  
28  
29 355 27]. It has been shown that the amplitude velocity of the CA decreases rapidly when the  
30  
31 356 system is altered by, for example, draining its fluid, and that this operation causes also alters  
32  
33 357 the phase of the tympana associated tympana [27]. However, the decrease in TW  
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35 358 wavelength with increasing frequency, and the corresponding increase in TW velocity,  
36  
37 359 presented here is in good agreement with predictions of TW function as observed in  
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39 360 vertebrate [1, 39] and invertebrate [6, 7] models.  
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41  
42 361 Understanding hearing processes such as tonotopy and TWs in mammals is crucial to  
43  
44 362 further auditory research regarding nonlinear processes within the cochlea [13]. As  
45  
46 363 mentioned before, anatomical limitations for accessing and obtaining data *in vivo*, and in an  
47  
48 364 intact system, has been a major drawback in this field. Recently, methods for the  
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50 365 measurement of auditory activity *in vivo* have improved notably for mammals.  
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52 366 Developments with various techniques using optical coherence tomography (OCT), provides  
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54 367 a visual technique for depth-resolved displacement measurements of TWs through the bony  
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56 368 shell that protects the cochlea [12, 40]. Although such OCT techniques appear to be non-  
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58 369 invasive, it still requires the middle ear bulla to be surgically treated to allow visual access to  
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4 370 the cochlea. This highlights the importance of developing novel and non-invasive techniques  
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6 371 for the acquisition of TW data, as an important part of the complex auditory system.  
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8 372 Attempts to relate the biomechanical tonotopy to the frequency tuning of the corresponding  
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10 373 sensory cells in bush-crickets have produced important advances in this field [23], and the  
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12 374 methodology presented here provides an opportunity for refinement of currently accepted  
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14 375 experimental protocols. The reduced number of auditory sensory neurons, and the short  
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16 376 length of the CA in theory compromises frequency resolution in the bush-cricket ear [7, 30,  
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18 377 42]. But certainly, these systems are not well understood and until the problem is rigorously  
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20 378 approached, the phenomena of frequency resolution and sensitivity will remain elusive.

## 21 22 23 379 **5. Conclusion**

24  
25 380 The transparent cuticle effectively supports the visualization and measurement of the  
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27 381 auditory activity with no manipulation of the hearing organ required. The main advantage of  
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29 382 this approach is that it overcomes the need for surgical intervention (i.e. removing the  
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31 383 cuticle). Additionally, the ability to image through the cuticle provides the opportunity for  
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33 384 experimental manipulation, such as the use of voltage-sensitive dyes to follow neuron  
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35 385 activity in real time of the mechano-sensory cells involved in the hearing process [43-45].  
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37 386 Furthermore, from the point of view of invasive experimental protocols, invertebrates, and  
38  
39 387 especially insects, are ideal substitutes within the 3Rs framework [46]. This work achieves  
40  
41 388 not only *replacement*, by providing a possible alternative to vertebrate models, but also  
42  
43 389 *refinement*, by using intact systems and noninvasive measurement, As animals are  
44  
45 390 unharmd during measuring, this has the potential to also *reduce* animal usage.

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47  
48 391 The bush-cricket inner ear is functionally and structurally less complex, yet smaller than  
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50 392 those of mammals. For instance, the number of mechano-sensory cells is considerably  
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52 393 lower in bush-crickets. Even so, the physical principals underlying hearing in mammals are  
53  
54 394 the same for hearing in bush-crickets [41]. The bush-cricket frequency analyser organ (the  
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56 395 CA-AV) is uncoiled and the tonotopic organization takes place in a relatively short distance  
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4 396 (approximately one third of the length of the mammalian basilar membrane), and individual  
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6 397 cap cells are visible on the surface of the tectorial membrane along the CA (figure S3). Such  
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8 398 features provide unprecedented opportunity for experimental manipulation and, by the  
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10 399 methodology presented here, for the collection of high-quality data. For example, a tentative  
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12 400 application of such studies would be the investigation of an analogous mechanical origin of  
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14 401 the TWs observed in the cochlea, and currently two hypotheses has been proposed to  
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16 402 explain this phenomenon. Firstly, that TWs arise from anisotropic properties of the basilar  
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18 403 membrane, resulting in tonotopically arranged displacement maxima causing excitation of  
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20 404 the sensory cells [1]. And secondly, that the observed TW is a by-product of independently  
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22 405 resonating sensory cells, coupled by a tectorial membrane [47]. We believe that this type of  
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24 406 study, and novel experimental designs, may open avenues of research which help answer  
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26 407 such fundamental questions in auditory mechanics, and could provide insights into the  
27  
28 408 evolution of acoustic perception, the likes of which cannot be attained by only investigating  
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30 409 mammalian models.

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32  
33 410 **Authors' contributions.** F.S-S. and F.M-Z., conceived and designed the experiments. F.S-  
34  
35 411 S. and B.C. performed the experiments. F.S-S., and C.D.S. analysed data. C.D.S. designed  
36  
37 412 all the statistical models. F.S-S., B.C. and F.M-Z. wrote the manuscript. All authors reviewed  
38  
39 413 the manuscript.

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7  
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532

**533 Ethics approval**

534 College of Science Research Ethics Committee (COSREC), University of Lincoln granted  
535 permission to conduct this research under number COSREC-2014-02, and authorised the  
536 participation of all researchers involved in this project.

**537 Data availability**

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538 Raw data for ear cuticle transparency (measured as transmittance), ear cuticle thickness,  
539 and measurement of travelling wave parameters (wavelength and velocity) have been stored  
540 in Dryad repository (DOI: doi:10.5061/dryad.cs4m9).  
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4 542 **Figure captions**

5 543 **Figure 1.** Study species and cuticle transmittance. (a) Species of bush-cricket (Tettigonidae)  
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7 544 used for the transmittance measurements. Top row habitus of the species, bottom row close  
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9 545 up view of the ear region showing the colour and level of cuticle pigmentation for each  
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11 546 species. Red circle indicates position of ear in bush-crickets. (b) Cuticle transmittance values  
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13 547 for all species studied. Transmittance curves (percentage of light diffused through the ear  
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15 548 dorsal cuticle [see also figure 2a]) measured in the visible light spectrum (370-800 nm). (c)  
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17 549 Mean transmittance values ( $\pm$  SE) of the ear dorsal cuticle of all species at the laser beam  
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19 550 wavelength (633 nm).

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22 551 **Figure 2.** Effect of cuticle transmission and thickness on LDV experiments. (a) Diagram of  
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24 552 experimental protocol for obtaining laser displacement ratios from freshly dissected ear  
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26 553 cuticle. See text for details. Image not to scale. (b) Relationship of cuticle transmittance,  
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28 554 cuticle thickness and laser displacement ratio.

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31 555 **Figure 3.** LDV experimental set-up and output. (a) Diagram of experimental protocol for non-  
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33 556 invasive measurements of auditory function in bush-crickets using LDV. See text for details.  
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35 557 Image not to scale. (b) Laser vibration map showing the distribution of areas of high vibration  
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37 558 amplitude. Inset: ear area scanned during the LDV experiments. (c) 3D representation of the  
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39 559 same data in *b* of a travelling wave at 10 kHz through phases of 45 degrees of the oscillation  
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41 560 cycle.

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44 561 **Figure 4.** Spatial frequency mapping and travelling waves in the inner ear of the glass bush-  
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46 562 cricket *Phlugis poecila*. (a) Close up view of the left leg ear showing a three-point transect on  
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48 563 between the anterior (ATM) and posterior tympanal membrane (PTM). The locations where  
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50 564 the maximum velocity were recorded in the ear for 19 kHz, 25 kHz, and 47 kHz are  
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52 565 represented by P1, P2, and P3 respectively. (b-d) Frequency response measured as velocity  
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54 566 gain at locations P1-P3. (e-g) Envelope reconstruction along the transect in A for 19 kHz, 25  
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56 567 kHz, and 47 kHz. The deflection envelopes are constructed by displaying phase increments  
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4 568 of 10° in the full oscillation cycle. The red colour broken line represents the phase lag in  
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6 569 degrees (red scale in the right) for the same frequencies and distance. (h) The velocity of the  
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8 570 travelling wave in *P. poecila*. (i) Travelling-wave wavelength in *P. poecila*.

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11 571 **Supplementary material captions**

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13 572 **Supplementary Figure 1.** Examples of cuticle dissections for quantification of cuticle  
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15 573 thickness. (a) Dorsal view of the ear, red line indicates location of cross section dissection.  
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17 574 (b) *Copiphora vigarosa*. (c) *Copiphora gorgonensis*. (d) *Phlugis poecila*. (e) *Acantheremus*  
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19 575 sp. (f) *Nastonotus foreli*.

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22 576 **Supplementary Figure 2.** Experimental set-up for non-invasively measuring travelling  
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24 577 waves in bush-crickets. See text for details. Inset: preparation of the mounted bush-cricket.

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27 578 **Supplementary Figure 3.** Cuticle transparency in a glass bush-cricket *Phlugis* sp. (a)  
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29 579 Lateral view of the femur, the acoustic trachea is clearly visible through the cuticle without  
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31 580 manipulation of the animal. (b) Dorsal view of the hearing organ. The cap cells (scolopidia)  
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33 581 are visible through the cuticle.

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38 583 **Supplementary Figure 4.** Acoustic analysis of the call of the two species exhibiting more  
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40 584 cuticle light transmittance. (a-c) *Phlugis poecila* and (d-f) *Copiphora gorgonensis*. (a) Typical  
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42 585 presentation of the call. (b) A single phonatome (closing stroke of the wings) in detail. (c)  
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44 586 Spectral analysis of the phonatome in (b). Wide bandwidth of prevalent frequencies are  
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46 587 apparent in the call of *P. poecila*. (d) Typical presentation of the call. (e) A single phonatome  
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48 588 (closing stroke of the wings) in detail. (f) Spectral analysis of the phonatome in (e). Note  
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50 589 higher tonal purity and harmonic content in the call of *C. gorgonensis*.

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56 591 **Supplementary Movie S1.** A video of the laser Doppler response of the crista acustica to a  
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58 592 10 kHz pure tone sound stimulus at 60 dB SPL. The animation is the resulting interpolation  
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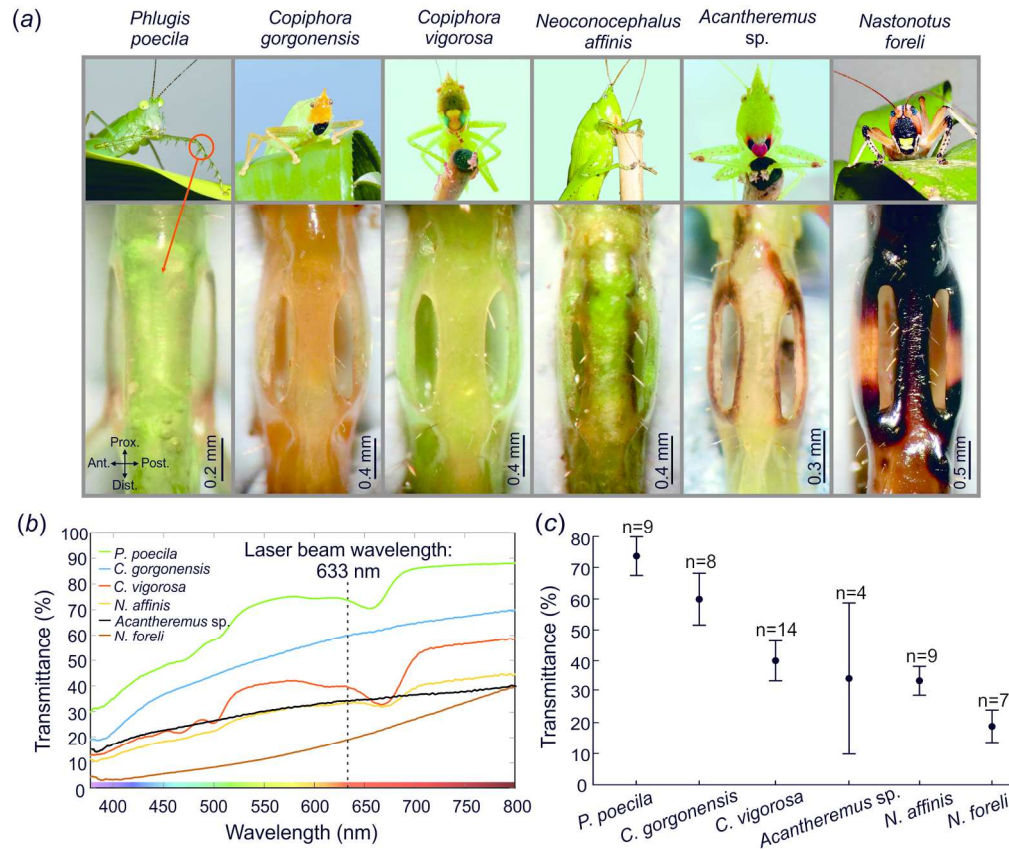
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4 593 of the measured points of the scanning grid. In the dorsal and side view of the ear, the  
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6 594 motion occurs in a distal to proximal direction (from the bottom to the top area of the video  
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8 595 and from left to right).  
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Figure 1. Study species and cuticle transmittance. (a) Species of bush-cricket (Tettigonidae) used for the transmittance measurements. Top row habitus of the species, bottom row close up view of the ear region showing the colour and level of cuticle pigmentation for each species. Red circle indicates position of ear in bush-crickets. (b) Cuticle transmittance values for all species studied. Transmittance curves (percentage of light diffused through the ear dorsal cuticle [see also figure 2a]) measured in the visible light spectrum (370-800 nm). (c) Mean transmittance values ( $\pm$  SE) of the ear dorsal cuticle of all species at the laser beam wavelength (633 nm).

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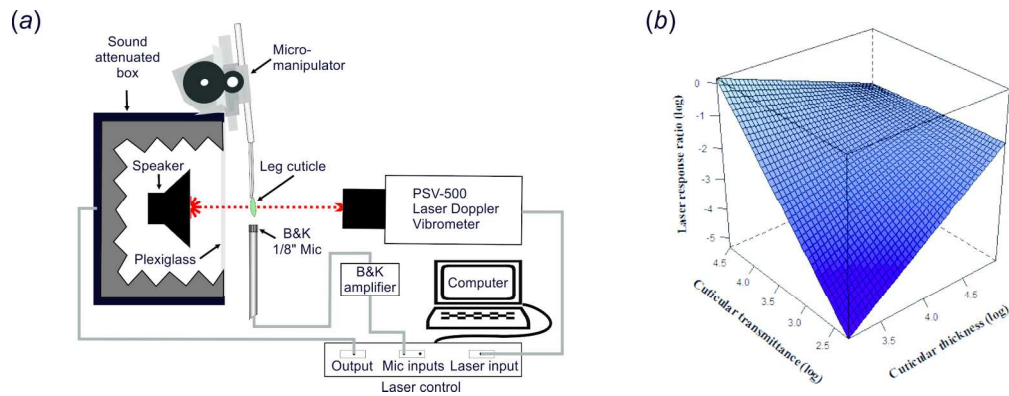


Figure 2. Effect of cuticle transmission and thickness on LDV experiments. (a) Diagram of experimental protocol for obtaining laser displacement ratios from freshly dissected ear cuticle. See text for details. Image not to scale. (b) Relationship of cuticle transmittance, cuticle thickness and laser displacement ratio.

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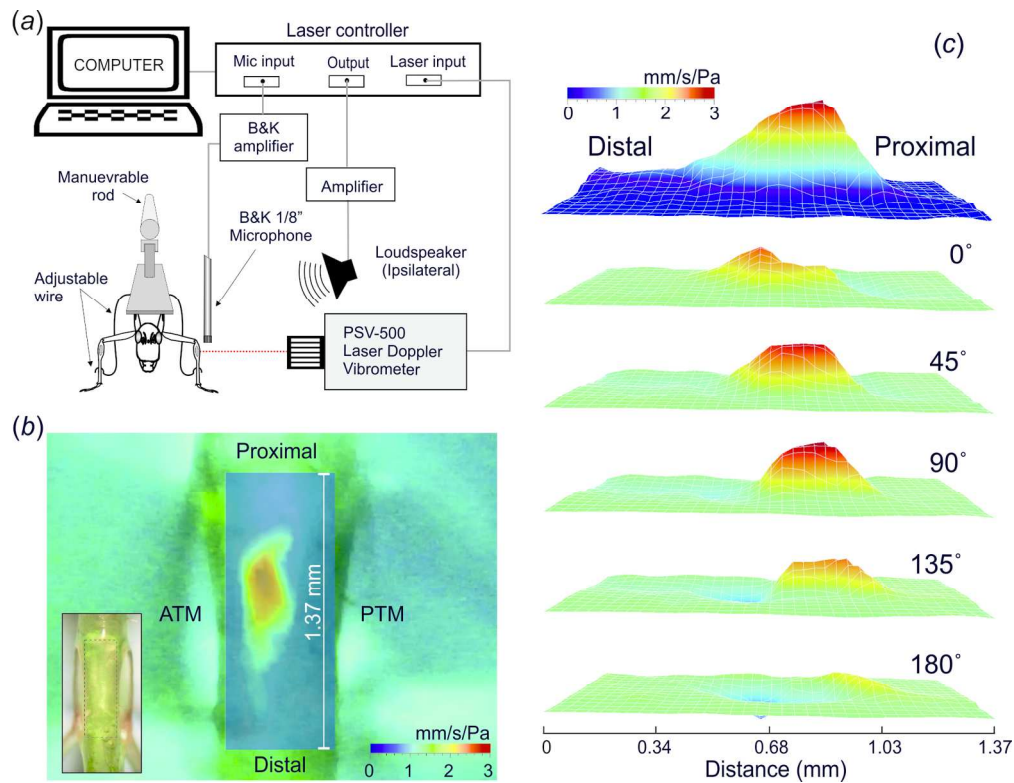


Figure 3. LDV experimental set-up and output. (a) Diagram of experimental protocol for non-invasive measurements of auditory function in bush-crickets using LDV. See text for details. Image not to scale. (b) Laser vibration map showing the distribution of areas of high vibration amplitude. Inset: ear area scanned during the LDV experiments. (c) 3D representation of the same data in b of a travelling wave at 10 kHz through phases of 45 degrees of the oscillation cycle.

Figure 4. Spatial frequency ma  
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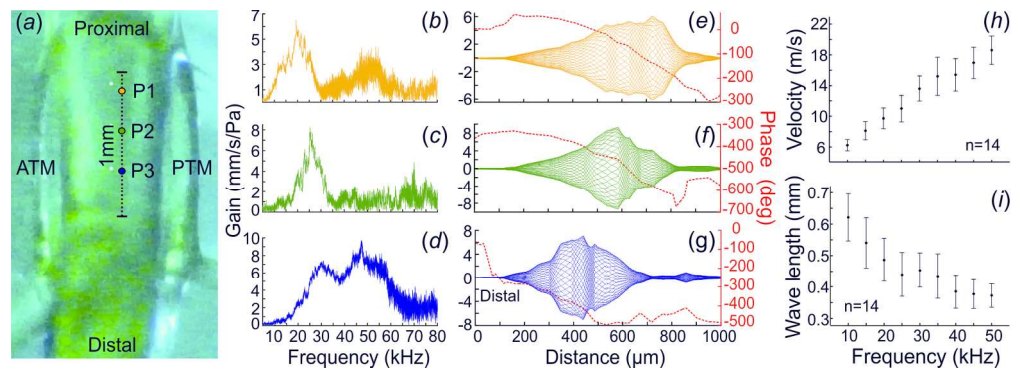


Figure 4. Spatial frequency mapping and travelling waves in the inner ear of the glass bush-cricket *Phlugis poecila*. (a) Close up view of the left leg ear showing a three-point transect on between the anterior (ATM) and posterior tympanic membrane (PTM). The locations where the maximum velocity were recorded in the ear for 19 kHz, 25 kHz, and 47 kHz are represented by P1, P2, and P3 respectively. (b-d) Frequency response measured as velocity gain at locations P1-P3. (e-g) Envelope reconstruction along the transect in A for 19 kHz, 25 kHz, and 47 kHz. The deflection envelopes are constructed by displaying phase increments of  $10^\circ$  in the full oscillation cycle. The red colour broken line represents the phase lag in degrees (red scale in the right) for the same frequencies and distance. (h) The velocity of the travelling wave in *P. poecila*. (i) Travelling-wave wavelength in *P. poecila*.

176x62mm (300 x 300 DPI)