

1 Title:

2 Comparison of subjective and objective methods to determine the retinal arterio-venous ratio  
3 using fundus photography

4

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25 Tables: 2

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28 Key words: retinal vessel diameters, arterio-venous ratio, central retinal artery equivalent,  
29 central retinal vein equivalent, reproducibility, semi-automated analysis, visual grading

30

1 **Abstract:**

2 Purpose: To assess the inter and intra observer variability of subjective grading of the retinal  
3 arterio-venous ratio (AVR) using a visual grading and to compare the subjectively derived  
4 grades to an objective method using a semi-automated computer program.

5

6 Methods: Following intraocular pressure and blood pressure measurements all subjects  
7 underwent dilated fundus photography. 86 monochromatic retinal images with the optic  
8 nerve head centred (52 healthy volunteers) were obtained using a Zeiss FF450<sup>+</sup> fundus  
9 camera. Arterio-venous ratios (AVR), Central Retinal Artery Equivalent (CRAE) and Central  
10 Retinal Vein Equivalent (CRVE) were calculated on three separate occasions by one single  
11 observer semi-automatically using the software VesselMap (ImedosSystems, Jena,  
12 Germany). Following the automated grading, three examiners graded the AVR visually on  
13 three separate occasions in order to assess their agreement.

14

15 Results: Reproducibility of the semi-automatic parameters was excellent (ICCs: 0.97  
16 (CRAE); 0.985 (CRVE) and 0.952 (AVR)). However, visual grading of AVR showed inter  
17 grader differences as well as discrepancies between subjectively derived and objectively  
18 calculated AVR (all  $p < 0.000001$ ).

19

20 Conclusion: Grader education and experience leads to inter-grader differences but more  
21 importantly, subjective grading is not capable to pick up subtle differences across healthy  
22 individuals and does not represent true AVR when compared with an objective assessment  
23 method. Technology advancements mean we no longer rely on ophthalmoscopic evaluation  
24 but can capture and store fundus images with retinal cameras, enabling us to measure  
25 vessel calibre more accurately compared to visual estimation; hence it should be integrated  
26 in optometric practise for improved accuracy and reliability of clinical assessments of retinal  
27 vessel calibres.

28

29

## 1 **Introduction:**

2 Assessing retinal vessel appearance including relative diameters is part of a standard ocular  
3 examination. Retinal vessel diameters have been shown to be valuable markers of systemic  
4 and ocular vascular complications in a range of pathologies including diabetes <sup>(1-3)</sup>,  
5 cardiovascular disease <sup>(4-6)</sup> and cerebrovascular complications <sup>(7, 8)</sup>. Despite the availability of  
6 a wide range of semi-automatic programs which can measure retinal arteriolar and venular  
7 diameters in order to calculate arterio-venous ratios (AVR), most optometrists still make a  
8 visual assessment.

9

10 Changes due to vascular abnormalities and those related to age are often subtle and can be  
11 overlooked when using visual grading systems. Most optometric practices are equipped with  
12 a digital fundus camera, typically used for diabetic retinopathy screening. Some of these  
13 software packages come with further image analyses options offering the possibility to  
14 measure retinal vessel diameters.

15

16 Visual grading systems in general exhibit poor reproducibility, low sensitivity and specificity  
17 as well as being highly dependent upon observer experience <sup>(9)</sup>. Changing observers/  
18 clinicians can lead to bias in analysing progression data, especially if observer variability is  
19 dependent on experience. Visual grading of arterio-venous ratio is almost binary in nature as  
20 it reflects a comparison of the relative diameter of retinal arteries to those of retinal veins.

21 There is a wide variety of literature and educational material used to teach clinicians and it is  
22 apparent that there is not only a lack of standardisation with respect to the measurement  
23 location but also in the numerical value of the ratio reflecting the “normal/ healthy” diameter  
24 relationship <sup>(10-12)</sup>. While some sources recommend comparison between vessels beyond the  
25 first bifurcation <sup>(10)</sup> others advise on the use of graticules superimposed on the Optic Nerve  
26 Head (ONH) <sup>(11)</sup> or to assess vessels only after their second bifurcation <sup>(12)</sup>. In stark contrast  
27 to this, semi-automated programs show a great deal of standardisation using a circular grid  
28 to measure vessel diameter only in a concentric ring segment one half disc diameter (DD)  
29 distant from the outer boundaries of the ONH and one half DD in width <sup>(13)</sup>. The formulae  
30 used to calculate AVR is based on the work of Parr, Spears and Hubbard <sup>(14-16)</sup> or its revised  
31 formulae published by Knudson et al in 2003 <sup>(13)</sup>. Clearly, for observations over a longer time  
32 period it seems obvious that a semi-automatic system is superior to visual grading, given  
33 that independent of the observer one can analyse identical vessel segments over time and  
34 there is greater precision in the measurement. The basis of an automated AVR is the  
35 application of an algorithm which includes measurement of the central retinal artery and  
36 central retinal vein diameter which results from the calculation of individual diameters of their

1 visible branches around the ONH <sup>(13)</sup>. Hence, subtle vascular changes may be identified  
2 earlier than is possible from visual assessment.

3 The objective of this research was threefold. *Firstly* we wanted to evaluate the influence of  
4 observer experience on visual grading and agreement between observers. *Secondly* we  
5 wanted to evaluate the reproducibility of a semi-automated program using fundus  
6 photographs of healthy Caucasian and South Asian individuals. The *final* objective was to  
7 evaluate how well visual grading agrees with the values derived using a semi-automated  
8 program.

## 1 **Materials and Methods:**

### 2 Subjects:

3 The study was approved by the Aston University Ethics Committee and followed the  
4 guidelines of the Declaration of Helsinki. All participants gave written informed consent prior  
5 to inclusion in the study. Fifty-two healthy individuals (age range: 20 – 61years) participated  
6 in the study. All participants initially underwent non-contact tonometry (Pulsair, Keeler, UK)  
7 followed by pupil dilation using one drop of tropicamide 1% (Bausch & Lomb, UK). After a  
8 minimum of 15-20 minutes acclimatisation in a temperature controlled room (21 degrees  
9 Celsius) systemic blood pressure and heart rate was measured using a digital  
10 sphygmomanometer (UA-767, A&D Instruments Ltd., UK). Once maximum pupil dilation was  
11 achieved, monochromatic (red free) retinal photographs were obtained using a Zeiss FF450+  
12 fundus camera with the ONH centred and the camera field angle set to 30 degrees.

13

### 14 Visual grading:

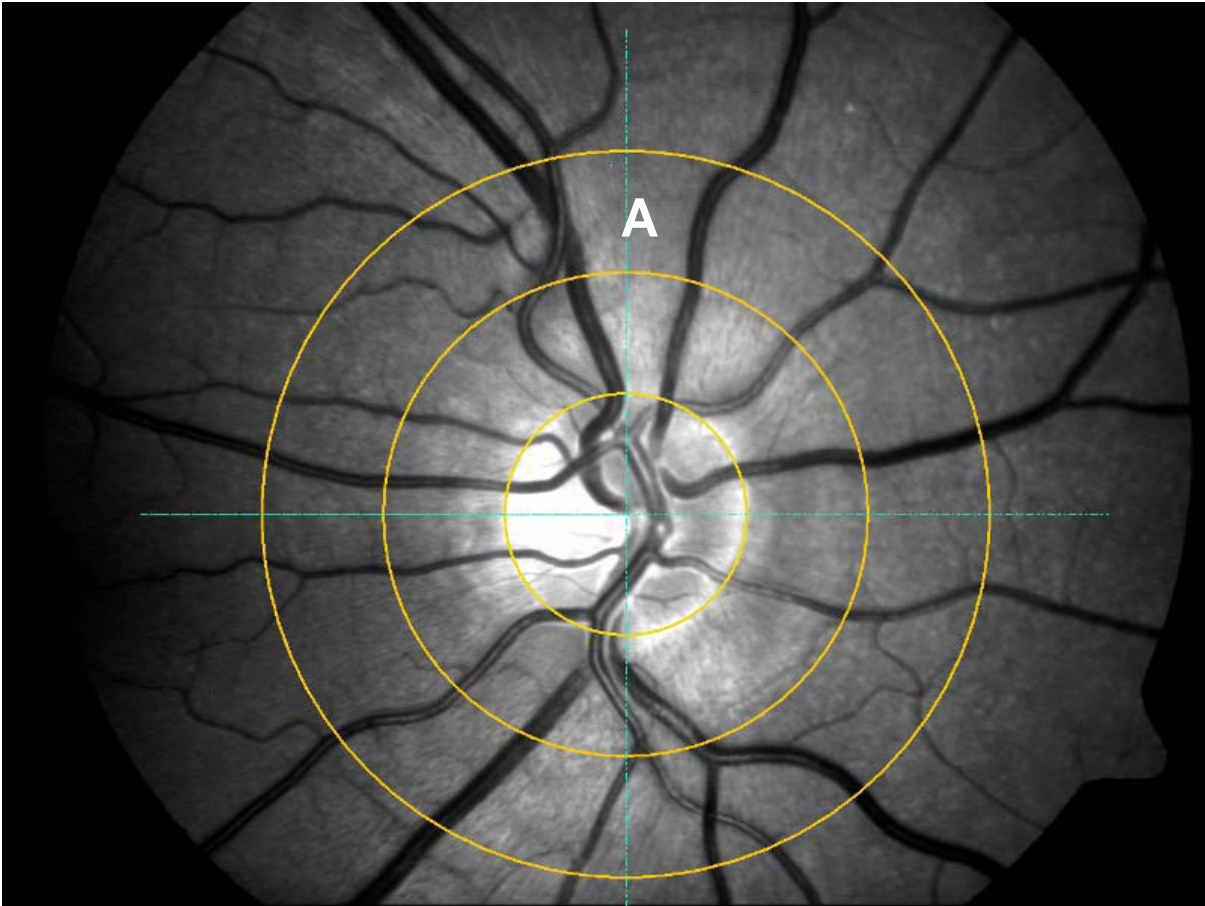
15 To explore the influence of experience and different educational training we asked three  
16 individuals to grade each image on three separate occasions. Each examiner was instructed  
17 to grade each image according to the way they would normally do so in clinical practice or as  
18 taught at University. Examiner 1 was a final year optometry student with little clinical  
19 experience, Examiner 2 was a fully qualified optometrist with 4 years clinical experience and  
20 Examiner 3 was a fully qualified optometrist with 20 years clinical experience.

21

### 22 Semi-automated grading:

23 Semi-automated grading was performed by a single observer grading each image on three  
24 different occasions using the Visualis software (ImedosSystems, Jena, Germany). In brief,  
25 following image selection a ring is placed around the ONH with 2 further concentric rings  
26 with each  $\frac{1}{2}$  DD and 1 DD distant from the ONH ring around it. The grader manually selects  
27 the six largest retinal arteries and veins passing through the outer ring segment A (see  
28 Figure 1) to include in the analysis (once the vessel is selected the analyses program  
29 recognizes the vessel and includes it's diameter in the calculation-no manual calliper  
30 selection is required); in cases of vessels branching in this segment, the vessel trunk was  
31 included but not its branches.

32



1

2 Figure 1: Illustrating an example of the images used for grading. The two out rings enclose  
3 the measurement area A in which all vessel diameters were included for further processing.

4

#### 5 Statistical analysis:

6 All data was analysed using STATISTICA version 6.0 (Statsoft, Tulsa, OK). All demographic  
7 and pressure data was normally distributed (Shapiro Wilk test). Intra-grader variability was  
8 assessed by calculating the Intra-class correlation coefficients (ICC) and Friedman's  
9 ANOVA, the software algorithm reproducibility was evaluated by calculating the ICC for  
10 each: CRAE, CRVE and AVR. All ICCs were calculated using a two-way mixed, absolute  
11 agreement, single measures model. More detail on the calculation and different models used  
12 to obtain ICCs can be found elsewhere <sup>(17)</sup>. Between grader and software AVR values were  
13 compared using Friedman's ANOVA followed by Wilcoxon signed rank test. Statistical  
14 significance was defined as  $p < 0.05$ .

15

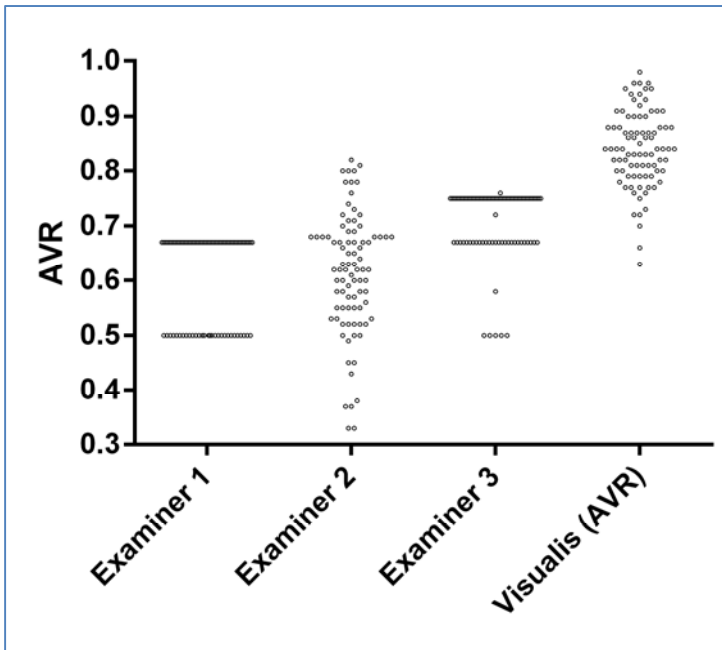
16

1 **Results:**

2 Eighty-six retinal photographs of 52 participants (mean age 30 SD 9 years) were included for  
 3 semi-automated vessel diameter assessment and subjective visual grading by three different  
 4 examiners. Systemic circulatory and Intraocular Pressure (IOP) values were within normal  
 5 limits for all participants (IOP: 12 (3) mmHg, systolic blood pressure: 114 (13) mmHg,  
 6 diastolic blood pressure: 70 (10) mmHg, heart rate: 68 (9) bpm).

7

8 *Influence of observer experience and agreement of visual and software generated grading:*

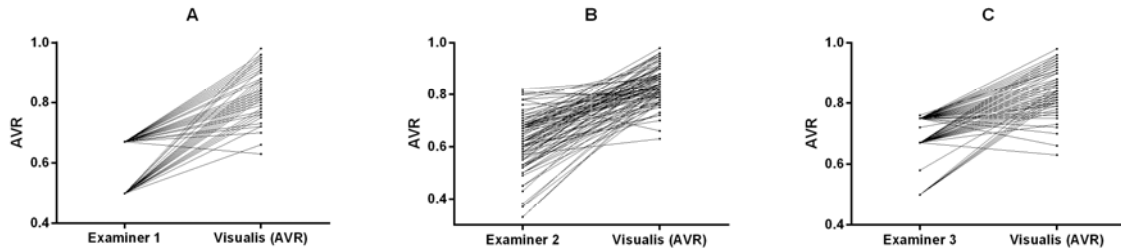


9

10 Figure 2: Illustrates the averages for AVR of all three examiners and the results obtained by  
 11 using the Visualis software (ImedosSystems, Jena, Germany). Each point denotes a single  
 12 grading.

13

14 While examiner 1 and 3 apply an almost binary grading system, examiner 2 uses a more  
 15 continuous approach. Despite the discrepancy between the examiners, on average all three  
 16 underestimate AVR when compared to the quantitative software based measurement. When  
 17 using a paired t-test to compare the results of the visual grading between examiners  
 18 numerically, only examiner 3 differs from both examiner 1 and 2 ( $p < 0.0000001$  and  
 19  $p < 0.0000001$  respectively). While a paired t-test is not suitable to assess examiner  
 20 differences, ICCs or correlations are not ideal (but for completeness can be found in table 2)  
 21 for comparison due to the non-continuous nature of this data; hence we chose to plot a  
 22 case-by-case graph connecting the results of the visual grading of each case for each  
 23 examiner and the automatic grading for better illustration (see Figure 3 below).



1

2 Figure 3: Illustration of case by case comparison for each examiner (average AVR) and the  
3 automated grading (average AVR).

4

<b>n=70</b>	<b>Examiner 1 AVR</b>	<b>Examiner 2 AVR</b>	<b>Examiner 3 AVR</b>	<b>Software AVR</b>
<i>Visual Grading</i>	<i>Mean (SD)</i>	<i>Mean (SD)</i>	<i>Mean (SD)</i>	<i>Mean (SD)</i>
AVR 1	0.61 (0.08)	0.59 (0.11)	0.71 (0.07)	0.84 (0.08)
AVR 2	0.61 (0.08)	0.63 (0.13)	0.71 (0.07)	0.84 (0.07)
AVR 3	0.61 (0.08)	0.62 (0.13)	0.71 (0.07)	0.84 (0.07)
Average AVR	0.60 (0.08)	0.61 (0.11)	0.71 (0.07)	0.85 (0.07)
Friedman's ANOVA p	0.606	0.097	0.717	0.405

5 Table 1: Grading results for all examiners and software derived grading. AVR 1: arterio-  
6 venous ratio grading 1, AVR 2: arterio-venous ratio grading 2, AVR 3: arterio-venous ratio  
7 grading 3, CRAE: central retinal arterial equivalent, CRVE: central retinal venous equivalent

8

### 9 Reproducibility of visual arterio-venous grading

10 To assess visual grading reproducibility of each grader we calculated the ICC comparing  
11 each graders second and final measurement.

Subjective AVR			
	Caucasian ICC	South Asian ICC	Both ethnicities ICC
Examiner 3	1	0.956	0.889
Examiner 2	0.480	0.644	0.556
Examiner 1	1	1	1

12 Table 2: Showing results of intra grader reproducibility. AVR: Arterio-venous ratio; ICC:  
13 Intraclass correlation coefficient.

14

15



1 Reproducibility of semi-automated arterio-venous parameter in Caucasian and South Asian

2 Individuals:

3 Reproducibility of automated arterio-venous parameter was excellent for both Caucasian  
4 and South Asian fundi. ICCs for Caucasian retinas [n=46] was 0.963 for AVR, 0.982 for  
5 CRAE and 0.988 for CRVE; similarly ICCs for South Asian retinas [n=40] was 0.927 for  
6 AVR, 0.95 for CRAE and 0.976 for CRVE.

7

8 Visual grading of AVR vs semi-automated AVR calculation:

9 To compare subjective AVR assessment with objective, software based AVR calculation we  
10 computed a Friedman's ANOVA which shows a significant difference ( $p < 0.000001$ ). As this  
11 is a non-parametric test we used the Wilcoxon signed rank test to compare each subjective  
12 grading with the semi-automated AVR. All subjective grading were significantly lower than  
13 the semi-automatically derived AVR (all  $p < 0.000001$ ).

14

1 **Discussion:**

2 Although individual grader reproducibility was good, there were marked differences between  
3 the three graders. Whilst examiner 1 and 3 were using an almost binary approach to grading  
4 the images, Examiner 2 showed a more continuous approach.

5

6 The differences between graders are most likely due to their clinical experience and  
7 University training. Examiners 1 and 2 were taught that a normal AVR is 2:3. Conversely,  
8 examiner 3 was taught that a normal AVR is 3:4 which explains in part the higher values of  
9 Examiner 3. Of note is also the marked binary grading of Examiner 1 compared to Examiner  
10 3. They are both using a binary approach but the differences between the two gradings are  
11 more subtle, probably due to the difference in clinical experience between examiners and  
12 that differences between subjects are very subtle and difficult to judge subjectively. When  
13 comparing the subjective grades of the examiners with the objective outcomes of the semi-  
14 automatic analysis it was apparent that a large discrepancy between visual and semi-  
15 automatic grading exists. Despite inter-grader differences, all examiners significantly  
16 underestimated AVR compared to the software generated output.

17

18 While AVR has shown to be a useful marker in vascular disease<sup>(18-20)</sup> this data highlights the  
19 inconsistencies and lack of clinical agreement with objective data for AVR. The further  
20 advantage of objective analysis of AVR is that it can be used for follow up visits and long  
21 term observations making it beneficial in a clinical environment.

22

23 As many of these programs have been developed and tested in Caucasian individuals we  
24 wanted to explore how robust the software algorithm is when repeating the measurement  
25 procedure using the same image on three separate occasions on Caucasian and South  
26 Asian retinal photographs. Our results show excellent reproducibility of software generated  
27 values for CRAE, CRVE and AVR in both ethnic groups. The slightly lower ICC values for  
28 AVR and CRAE in the South Asian fundi is most likely due to the inherent lower contrast of  
29 the photographic images.

30

31 AVR as a standalone measurement is of limited clinical use as in the context of diagnosis it  
32 is advantageous to identify whether vessel diameters have altered because of venous,  
33 arterial changes or both<sup>(21, 22)</sup>. The existing subjective grading method is limited since an  
34 alteration of the AVR from for example 2:3 to 1:2 is commonly referred to as retinal arteriolar  
35 narrowing, but the same ratio will be achieved by venous dilation, commonly encountered in  
36 diabetic retinopathy. More clinically useful measures for monitoring are the CRAE and CRVE  
37 indices which can only be achieved using automated analysis.

1 Publications on the utility, clinical validity and applications for retinal vessel diameters are  
2 numerous but to date not widely integrated into clinical practice. For example, Liew and  
3 colleagues reported retinal vessel parameter of a subset of participants from the  
4 Atherosclerosis Risk in Communities (ARIC) study (n=8794) showing that the major  
5 systemic determinant for smaller CRAE is higher blood pressure whereas wider CRVE is  
6 mainly due to current cigarette smoking, higher blood pressure, systemic inflammation and  
7 obesity. Those with higher blood pressure (75<sup>th</sup> percentile) had on average 4.8 microns  
8 smaller CRAE and 2.6 microns wider CRVE than those with lower blood pressure (25<sup>th</sup>  
9 percentile)<sup>(23)</sup>. More recent work by Daien and colleagues found a strong negative correlation  
10 between renal function and retinal parameters (CRAE and CRVE) in a cohort of eighty  
11 healthy individuals which suggests a common determinant in pre-clinical target organ  
12 damage <sup>(24)</sup>. This is in support of earlier studies<sup>(25,26)</sup>, examining the association between  
13 retinal vascular signs and incident hypertension providing evidence that a decrease in CRAE  
14 is indeed an antecedent to clinical onset of hypertension and occurs prior to other signs of  
15 target organ damage.

16 Besides the value of CRAE in predicting hypertension, it also shows great potential in other  
17 pathologies including stroke and diabetes. Generalised arteriolar narrowing as reflected by a  
18 decrease in CRAE is associated with an increased risk in stroke <sup>(27-29)</sup>. While in diabetes an  
19 increase of CRVE was associated with increased incidence of diabetic retinopathy (DR),  
20 progression of DR, progression to proliferative DR and macular oedema <sup>(30)</sup> but was  
21 unrelated to CRAE.

22 Apart from its potential for risk prediction, screening and monitoring systemic pathologies,  
23 retinal vessel parameter have been shown to be of clinical value in ocular vascular  
24 abnormalities such as glaucoma and AMD. Results of the Handan Eye Study showed the  
25 association of increased CRAE with early AMD <sup>(31)</sup>, while an increased risk of open angle  
26 glaucoma (OAG) was associated with a decrease in CRAE <sup>(32)</sup>.

27

28 In conclusion, the retinal circulation is an ideal vascular bed to observe changes non-  
29 invasively. Although we thoroughly assess its structure, vasculature and overall appearance,  
30 this is mostly done by subjective visual assessment despite the wide use of fundus cameras.  
31 A steep increase of patients at risk and/or suffering from cardiovascular diseases such as  
32 hypertension, diabetes and heart disease paired with an increasingly older population brings  
33 about an increased necessity for screening and monitoring. Optometrists already play an  
34 integral part in the screening of DR and with the strong evidence of retinal vessel parameters  
35 association with systemic and ocular pathology these markers might provide enhanced  
36 diagnostic/ prognostic power in existing pathology (hypertension and diabetes) and for those  
37 at risk of developing future ocular vascular pathology. While retinal vascular changes

1 themselves do not always lead to immediate loss in visual function, they are useful markers  
2 for future risk. Any measurement/ assessment a patient has to undergo should be of clinical  
3 use, AVR as determined by subjective grading is an out-dated measure which has been  
4 superseded by objectively determined diameter measurements. Regular retinal photography  
5 as part of a standard eye examination is becoming a reality as cameras and computer power  
6 have increased rapidly and made imaging technology an affordable tool for everyday clinical  
7 practice.

8 Consequently, the implementation of automated AVR measurements would provide a much  
9 more reliable tool to monitor vascular changes as part of a routine eye examination. Current  
10 optometry practice places more emphasis on diagnosis and monitoring of both ocular and  
11 systemic diseases rather than the provision of screening. Optometry practice already has the  
12 technological infrastructure to implement such changes, but there is perhaps a need to  
13 update professional guidelines and educational training in the measurement and clinical  
14 utility of AVR, CRAE and CRVE measurement in order to improve the clinical utility of this  
15 aspect of fundus examination.

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