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2 Original article

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4 Sheltering DNA in self-organizing, protein-only nano-shells as artificial viruses for gene  
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40

41 **Abstract**

42 By recruiting functional domains supporting DNA condensation, cell binding,  
43 internalization, endosomal escape and nuclear transport, modular single-chain  
44 polypeptides can be tailored to associate with cargo DNA for cell-targeted gene  
45 therapy. Recently, an emerging architectonic principle at the nanoscale has permitted  
46 tagging protein monomers for self-organization as protein-only nanoparticles. We have  
47 studied here the accommodation of plasmid DNA into protein nanoparticles assembled  
48 with the synergistic assistance of end terminal poly-arginines (R9) and poly-histidines  
49 (H6). Data indicate a virus-like organization of the complexes, in which a DNA core is  
50 surrounded by a solvent-exposed protein layer. This finding validates end-terminal  
51 cationic peptides as pleiotropic tags in protein building blocks for the mimicry of viral  
52 architecture in artificial viruses, representing a promising alternative to the conventional  
53 use of viruses and virus-like particles for nanomedicine and gene therapy.

54

## 55 **Background**

56 Non-viral gene therapy and in general emerging nanomedicines aim to mimic viral  
57 activities in tuneable nanoparticles, for the cell-targeted delivery of cargo nucleic acids  
58 and other drugs [1;2]. Among a diversity of tested materials (including lipids, natural  
59 polymers, quantum dots, carbon nanotubes and dendrimers), proteins offer full  
60 biocompatibility, biodegradability, and a wide spectrum of functionalities that can be  
61 further adjusted by genetic engineering. Such a functional versatility is in contrast with  
62 the null control so far exercised over the supramolecular organization of *de novo*  
63 designed building blocks for protein-based complexes [3]. While protein nanoparticles  
64 based on natural cages, mainly infectious viruses [4], virus-like particles (VLPs) [5],  
65 eukaryotic vaults [6] and bacterial microcompartments (BMCs) [7] take advantage of  
66 the evolutionarily optimized self-assembling activities of their building blocks, fully the  
67 *de novo* multifunctional protein monomers fail to reach predefined nanoscale organization.  
68 Only a very limited number of approaches, based on the engineering of oligomerization  
69 domains present in nature have resulted in the successful construction of efficient  
70 building blocks for protein shell generation [8]. Complexes of DNA and cationic proteins  
71 often result in polydisperse soluble aggregates probably derived from intrinsically  
72 disordered protein-protein interactions [9;10], or in which the DNA itself plays a leading  
73 architectonic role, stabilizing aggregation-prone protein monomers in form of  
74 monodisperse nanoparticles [11]. Self-assembling peptides, that organize as different  
75 types of nanostructured materials [12], promote unspecific aggregation when fused to  
76 larger proteins [13;14], making them useless as fine architectonic tags. In summary,  
77 the rational *de novo* design of protein monomers with self-assembling activities has  
78 remained so far unreachable. Very recently [15], we have described that pairs of  
79 'architectonic' peptides consisting of an N-terminal cationic stretch plus a C-terminal  
80 polyhistidine, when combined in structurally diverse scaffold proteins (GFP, p53 and  
81 others), generate strongly dipolar charged monomers that spontaneously self-  
82 assemble. The resulting protein oligomers, ranging from 10 to 50 nm, show fast nuclear

83 migration (compatible with cytoskeleton-linked active transport) and penetrability [16],  
84 high stability and proper biodistribution upon systemic administration [17]. Important  
85 levels of gene expression were also achieved when the protein was associated to  
86 plasmid DNA [18]. Yet these protein particles efficiently bind plasmid DNA for  
87 transgene expression and are very promising tools in nanomedicine [18], their  
88 supramolecular organization remains so far unexplored. The purpose of this study is to  
89 investigate the architectonic properties of the polyplexes formed by expressible DNA  
90 and the paradigm protein R9-GFP-H6, to better understand the basis of the high cell  
91 penetrability and at which extent the resulting complexes adopt virus-like organization.  
92 A solid comprehension of how multifunctional proteins interact with exogenous DNA  
93 should enable the design and efficient biofabrication of true artificial viruses.

94

## 95 **Methods**

### 96 Protein production and DNA binding

97 The modular organization of R9-GFP-H6 [18], T22-GFP-H6 [17] and HNRK [11] has  
98 been described elsewhere. GFP-H6 is a parental version of R9-GFP-H6 and T22-  
99 GFP-H6 that does not self-assemble under physiological conditions [15;18]. Apart  
100 from their architectonic capability, R9 (RRRRRRRRR) acts as a cell penetrating  
101 peptide and nuclear localization signal [18] and T22 (RRWCYRKCYKGYCYRKCR) as  
102 a powerful ligand of the cell surface receptor CXCR4 [17]. Both stretches, being  
103 cationic, are potentially able to bind DNA. H6 (HHHHHH) is at the same time a useful  
104 tag for one-step chromatographic protein purification and a potent endosomolytic  
105 agent [19]. Precise amino acid sequences at the links between GFP and the fused  
106 peptides can be found elsewhere [17]. The protein constructs indicated above were  
107 produced in bacteria following conventional procedures and purified in a single step by  
108 His-based affinity chromatography [15], through activities assisted by the Protein  
109 Production Platform (CIBER-BBN) ([http://www.bbn.ciber-](http://www.bbn.ciber-bbn.es/programas/plataformas/equipamiento)  
110 [bbn.es/programas/plataformas/equipamiento](http://www.bbn.ciber-bbn.es/programas/plataformas/equipamiento)). Protein-DNA complexes were

111 generated by incubation at appropriate ratios in HBS buffer (pH 5.8) for 60 min at  
112 room temperature.

113

114 Cell culture, confocal microscopy and transmission electron microscopy (TEM)

115 HeLa (ATCC-CCL-2) cell line was cultured as previously described [16] and always  
116 monitored in absence of fixation to prevent internalization artefacts. Nuclei were  
117 labelled with 200 ng/ml Hoechst 33342 (Molecular Probes, Eugene, Oregon, USA)  
118 and plasma membranes with 2.5 µg/ml CellMask™ Deep Red (Molecular Probes,  
119 Invitrogen, Carlsbad, CA, USA) for 5 min. Cells exposed to nanoparticles were  
120 recorded with a TCS-SP5 confocal laser scanning microscope (Leica Microsystems,  
121 Heidelberg, Germany) with a Plan Apo 63x / 1.4 (oil HC x PL APO lambda blue)  
122 objective. Three-dimensional cell models were generated with the Imaris v. 6.1.0  
123 software (Bitplane; Zürich, Switzerland). For TEM, protein/DNA complexes were  
124 contrasted by evaporation of 1 nm platinum layer in carbon-coated grids and then  
125 visualized in a Hitachi H-7000 transmission electron microscope.

126

127 DNA protection assay

128 In the buffers optimal for their respective stability [11;15], R9-GFP-H6 and GFP-H6  
129 (HBS pH 5.8), T22-GFP-H6 (carbonate buffer, pH 5.8) and HNRK (HBS + dextrosa pH  
130 5.8) were mixed with 1 µg of plasmid DNA (pTurboFP635, [18]) at 1 and 2 retardation  
131 units. Mixtures were incubated at room temperature for 1 h and then treated with 0.5  
132 µg/ml DNase I (Roche) at 37° C, in presence of 2.5 mM MgCl<sub>2</sub> and 0.5 mM CaCl<sub>2</sub>.  
133 Samples were collected just before DNase I addition and at 5, 20 and 60 min of the  
134 digestion reaction. DNase I was inactivated by adding EDTA 2.3 µM final  
135 concentration and by heating the samples for 20 min at 70° C. The remaining DNA  
136 was released from protein complexes by adding 10 U of Heparin followed by 2 hours  
137 incubation at 25° C. Subsequently, samples were analyzed in 1% agarose gels. DNA

138 signals in agarose gel were interpreted and analyzed with Quatity One software (Bio-  
139 Rad). Experiments were performed by triplicate.

140

141 Determination of particle size and Z potential

142 Volume size distributions of self-assembled protein nanoparticles and protein-DNA  
143 complexes were determined by triplicate using a dynamic light scattering (DLS)  
144 analyser at the wavelength of 633 nm, combined with non-invasive backscatter  
145 technology (NIBS) (Zetasizer Nano ZS, Malvern Instruments Limited, Malvern, U.K.). Z  
146 Potencial of these materials was determined in the same device in HBS buffer (pH 5.8,  
147 10 µg/mL final protein concentration). Measurements were carried out at 25 °C using a  
148 disposable plastic cuvette. Each sample was analysed by triplicate.

149

150 Molecular modelling

151 To build R9-GFP-H6-based particles, a model of the monomer was first generated  
152 using Modeller 9v2 [20] and the pdb structure "1qyo" as template. The arginine and  
153 histidine tails were modeled using the loopmodel function of this package. The  
154 structural models of the assembled monomers at pH 7 and pH 5.8 were then created  
155 using HADDOCK 2.0 [21], with the protonation states chosen according to pH and  
156 residue pKas, defining the 9 arginines at the N-terminus as active residues and the 6  
157 histidines at the C-terminus as passive residues and enforcing C5 symmetry led to  
158 star-shaped conformations. Alternative conformations were obtained using the tail  
159 arginines as active residues and no passive ones. All these models where analysed  
160 with FoldX using the function "AnalyseComplex" [22]. Defaults were taken for any  
161 other simulation parameters. This protocol has been already used in a previous study  
162 [18]. DNA was modeled for a 26 bp random sequence with the 3DDART server [23]  
163 using default parameters. The structural model of the (1:1) DNA-protein complex was  
164 created with HADDOCK2.0 using N-terminal-tail arginines and C-terminal-tail  
165 histidines as active residues and all DNA bases as passive ones. Superposition of all

166 resulting solutions was performed with PROFIT [24] (an implementation of the  
167 McLachlan algorithm, [25]) , using only the DNA molecule as subject of the structural  
168 fit. The structural comparison of disks made of TMV coat protein and R9-GFP-H6 was  
169 performed with SwissPdbViewer\* [26] to superimpose the 2om3 PDB structure and  
170 the modelled building block [27]. To facilitate the visualization of the resulting models,  
171 images were generated using Chimera [28] as rendering tool.

172

### 173 **Results**

174 Hexahistidine tails, when combined in single chain polypeptides with N-terminal  
175 cationic peptides, such as R9 or T22, promote assembling of these building blocks as  
176 regular particles at neutral or slightly acidic pH values [15], at which the imidazol group  
177 gets protonated and the tag moderately cationic [19]. When nanoparticles formed by  
178 R9-GFP-H6 at pH 7 and 8 (Figure 1a) were incubated with DNA, particle size remained  
179 close to 20 nm (Figure 1 b), the size previously observed in absence of DNA [15]. At  
180 pH 4 and 10, protein-DNA complexes peaked at 0.8 and 2  $\mu$ m respectively (Figure 1 b),  
181 which is in agreement with the tendency of the protein alone to form amorphous  
182 aggregates under denaturing conditions Figure 1 a). Interestingly, at slightly acidic pH  
183 (5.8), where the transfection mediated by R9-GFP-H6 had resulted more efficient [15],  
184 the population of polyplexes split in two fractions, peaking at 38 and 700-800 nm  
185 respectively, with no symptoms of protein instability or aggregation (protein-only  
186 nanoparticles peaked between 20 and 30 nm). The ability of these protein constructs to  
187 bind DNA was generically confirmed by retardation mobility assays (Figure 1 c).

188

189 These polyplexes were examined by confocal microscopy during exposure to cultured  
190 cells, taking advantage of the natural green fluorescence of the protein partner and  
191 upon staining the DNA with the blue fluorescent dye Hoechst 33342. Small spherical  
192 particles (Figure 2 a) and larger rod-shaped versions, some slightly twisted or ramified  
193 (Figure 2 b) were observed, whose size fitted respectively to the two main peaks



194 determined by DLS (Figure 2 b). The blue DNA signal appeared coincident with the  
195 green label, but its slightly smaller size suggested that DNA occurred in inner cavities  
196 of protein entities. Qualitatively, rod-shaped nanoparticles seemed more efficient in  
197 embedding DNA than the regular versions, as an important fraction of spheres, but not  
198 rods, appeared to be empty (Figure 2 a, b). Fine confocal sections and 3D isosurface  
199 reconstructions strongly suggested that a core DNA was shielded by a solvent-exposed  
200 protein layer (Figure 2 c), in a virus-like architectonic scheme.

201

202 In this regard, rod-shaped forms shown in Figure 2 a and c strongly evoked the  
203 morphologies of capsid proteins observed in plant viruses. Furthermore, a  
204 superimposition of the RNA-containing, rod-shaped tobacco mosaic virus (TMV) disk (a  
205 structural intermediate in the construction of helical capsids) and an energetically  
206 stable, planar, star-shaped molecular model of the self-assembled R9-GFP-H6 at pH  
207 5.8 are presented (Figure 2 d), showing coincidence in diameter and in monomer  
208 organization. Interestingly, a similar spatial distribution of arginines around the central  
209 cavities was found in both viral and non-viral complexes (Figure 2 d, inset). TEM  
210 images of material deposited on the grid in absence of cells indicated again a  
211 prevalence of tubular structures (Figure 2 e), with a diameter compatible with the  
212 particles observed by confocal analyses (between 20 and 30 nm) and with R9-GFP-H6  
213 disks obtained by molecular modelling (Figure 2 d). Importantly, no DNA was found  
214 associated to internalized R9-GFP-H6 protein-only nanoparticles (Figure 2 f). This  
215 indicates that cellular nucleic acids that the protein complexes might eventually find  
216 during the intracellular trafficking would result not available for binding, and that the  
217 only cargo suitable to form artificial viruses is the nucleic acid loaded *in vitro*.

218

219 Furthermore, DNA embedded in R9-GFP-H6 shells resulted highly protected from  
220 DNase I attack (Figure 3 a). This effect was similar to that promoted by the closely  
221 related, self-assembling construct T22-GFP-H6. Contrarily, the short modular peptide

222 HNRK [18;29], that although being positively charged does not exhibit architectonic  
223 properties, failed in protecting DNA from digestion (Figure 3 a). In the HNRK-DNA  
224 polyplexes, from which DNA overhangs, the nucleic acid is the main architectonic  
225 regulator of the resulting particles (of around 80 nm), the protein fraction being  
226 clustered by DNA instead of entrapping it in shell-like structures [11]. The high  
227 protection of R9-GFP-H6-linked DNA also indicates that whether DNA molecules are  
228 externally associated to some protein particles as suggested by confocal analysis  
229 (Figure 2), the fraction of such material is statistically low.

230

231 Why at slightly acidic pH and in presence of DNA, R9-GFP-H6 ~20 nm-nanoparticles  
232 rearrange as alternative spherical or cylindrical shells remains to be solved, but it might  
233 be speculated that the dipolar nature of the modular protein would permit a  
234 reorganization of the building blocks, to orient the positive protein patches at the inner  
235 surface of the shell, in contact with DNA. For that, spheres and cylinders would permit  
236 appropriate protein-protein interactions. In agreement with this hypothesis, the  
237 superficial charge of protein-only particles was  $-16.2 \pm 1.8$  mV, while in presence of  
238 plasmid DNA (2 RU) it shifted to a more negative value ( $-24.5 \pm 2.0$  mV) (Figure 3 b).  
239 Interestingly, by applying the same amount of protein, the number of nanoparticles was  
240 reduced by more than 50 % in the presence of DNA, consistent with a higher protein  
241 demand to form nanoparticles up to 800 nm than to form protein-only nanoparticles of  
242 ~20 nm. On the other hand, the organization of protein shells as spheres or  
243 alternatively as rods would require a certain degree of flexibility in monomer-monomer  
244 contacts, allowing alternative arrangements of the oligomers. The in-equilibrium  
245 protonation and charge profile of the histidine tail population ( $pK \sim 6$ ) [19], would confer  
246 enough structural versatility of these interactions supportive of spherical and disk-  
247 based cylindrical organization. In agreement, alternative stable versions of R9-GFP-H6  
248 oligomers (pentamers) resulted from the docking process, sustained by slightly  
249 divergent styles of inter-molecular interactions (Figure 4 a). Such pentamers, similarly

250 distributed oligomers (eg hexamers) orf their combination, could support both spherical  
251 and rod-shaped architectures as in the case of virus shells. After careful analysis of  
252 these models, we have identified, apart from electrostatic interactions (-7.33 Kcal/mol),  
253 van der Wals forces as the main components keeping the monomers together (-42.38  
254 Kcal/mol), in some cases with hydrogen bonds (-29.13 Kcal/mol)  
255 contributing significantly to the stability of the oligomers (data taken from the model  
256 disk represented in Figure 1 d and in Figure 4 a, left).

257

258 Figure 4 b shows a potential mode of interaction between DNA and R9-GFP-H6, based  
259 on unspecific charge-charge interactions between DNA and the GFP-overhanging tails.  
260 This architecture would enable the organization of several GFP molecules around a  
261 single DNA helix in a form similar to those shown in Figure 2 d for RNA, as suggested  
262 by the superposition of the best 50 solutions of a (1:1) DNA-protein docking simulation,  
263 which shows a uniform distribution of GFP-based building blocks around the DNA.

264

## 265 **Discussion**

266 The severe biological risks and negative media perception associated to the  
267 administration of natural viruses [30] have dramatically compromised the development  
268 of viral gene therapy [31;32] and prompted researchers to explore manmade  
269 alternatives as vehicles for the delivery of therapeutic genes. The artificial virus concept  
270 [2] claims the use of nanoparticles, that upon convenient upstream design, biological  
271 fabrication and engineering can successfully mimic properties of the viral infectious  
272 cycle that are relevant to transgene delivery and expression [33]. Nanotechnologies  
273 and material sciences offer interesting approaches to generate functional  
274 nanostructured carriers, and a spectrum of materials are being explored in this regard  
275 [34], even under suspicion of potential toxicity [35]. Among them, proteins are the most  
276 versatile regarding structure and function, being fully biocompatible, suitable of  
277 biological fabrication and not posing safety of toxicity concerns. In fact, vaults and

278 BMCs, or the recombinant version of viruses, namely VLPs, can be conveniently  
279 adapted to embed cargo molecules for targeted delivery [36]. In a more versatile  
280 approach, modular proteins containing cationic stretches for nucleic acid binding and  
281 condensation, as well as other functional segments such as cell penetrating peptides,  
282 ligands or nuclear localization signals, have been under continuous design to recruit  
283 virus-like functions in single chain molecules [37-40]. However, despite the functional  
284 versatility of these constructs they fail to reach ordered nanoscale structures, in most  
285 cases being the DNA the main driving force of the polyplex architecture [11]. In fact,  
286 the assembly of viral capsids results from a complex combination of intermolecular  
287 interactions including hydrophobic, electrostatic, van der Waals, and hydrogen bonds  
288 [41] that are excluded from a rational design in the novo designed recombinant  
289 proteins. Recently, we have determined that a combination of a cationic peptide plus a  
290 hexahistidine, placed at the amino and carboxy termini respectively of modular proteins  
291 grant them with the ability to self-organize as regular protein-only nanoparticles, able to  
292 penetrate target cells and to reach the nucleus in a very efficient way [15-17]. We have  
293 here shown how at a slightly acidic pH and in presence of DNA, the contacts promoted  
294 by the hexahistidine tail are able to accommodate structural rearrangements, among  
295 others those promoting a re-orientation of cationic segments in the inner surface, that  
296 convert plain oligomers into more complex supramolecular structures, namely closed  
297 protein shells, in a virus-like fashion (Figures 1, 2). Both conventional isometric and  
298 rod-shaped architectonic models occurring in natural viruses are spontaneously  
299 reached by the self-assembling of tagged GFP-H6, efficiently embedding the foreign  
300 DNA in the inner cavity of a protein-only shell (Figure 2). Such a dual construction  
301 scheme at the nanoscale reminds the organization of viral proteins. The rotavirus VP6  
302 capsid protein, whose essential organization is a trimer, assembles into either  
303 nanotubes or nanospheres when produced as a recombinant version [42]. Cationic  
304 peptides R9 and H6 promotes the oligomerization of a monomeric GFP into particles  
305 whose size measured by DLS (Figure 1 a) is compatible with that of pentamers (or

306 eventually hexamers, Figure 4 a). The presence of exogenous DNA upon in vitro  
307 incubation stimulates the arrangement of these building blocks in higher order, larger  
308 complexes (Figure 1 b) with flexibility to form nanospheres and nanotubes (Figure 2).  
309 The organizing ability of DNA over cationic proteins to form ordered protein-DNA  
310 complexes has been reported previously ([11] and references therein), and cationic  
311 interactions seem to be the driving force for the primary DNA-protein interaction (Figure  
312 1 c), that result in nuclease attack protection (Figure 3). The ability of R9-GFP-H6  
313 oligomers to bind and combine with nucleic acids is restricted to exogenous DNA, as  
314 not protein-DNA complexes were observed when mammalian cells were exposed to  
315 protein alone, which efficiently internalizes cultured cells ([16] and Figure 2 f). In  
316 addition, the carrier DNA promotes important levels of gene expression, the whole R9-  
317 GFP-H6-DNA complexes acting structurally and functionally like artificial viruses.

318

319 Importantly, the ability of the end-terminal tags of cationic nature to promote protein  
320 self-assembling seems to be irrespective of the polypeptide chosen as the core of the  
321 assembly, or at least not limited to a particular protein species [15]. This opens a door  
322 to select non-immunogenic homologous protein candidates as building blocks of  
323 nanoparticles in order to avoid any immune response upon systemic administration,  
324 what could be a critical bottleneck to the therapeutic use of artificial viruses based on  
325 *de novo* designed self-assembling proteins.

326

327 In summary, we have demonstrated for the first time how protein-based artificial  
328 viruses, namely functional nanoparticles formed by self-assembling protein shells  
329 shielding a core DNA, can be generated by the fully *de novo* design of building blocks.  
330 This fact not only validates R9 and H6 as pleiotropic peptides in vehicles for non-viral  
331 gene therapy, but it also reveals an unexpected architectonic potential of these tags in  
332 the generation of tuneable protein shells, whose properties can be further polished by  
333 conventional protein engineering. These versatile agents are promising alternatives to

334 natural protein constructs, including viruses, VLPs, vaults and BMCs, which because of  
335 several limitations including rigid architecture but also biosafety concerns, are less  
336 suitable for engineering and adaptation to nanomedical purposes.

337

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466 **Figure 1.** Molecular architecture of R9-GFP-H6-DNA polyplexes. A) Size distribution of  
467 R9-GFP-H6 in absence of DNA, at different pH values. Some of the data shown here  
468 have been published previously [15]. B) Size distribution of R9-GFP-H6-DNA  
469 polyplexes formed at different pH values. DNA alone is shown as a control. C) DNA  
470 mobility assay (using pTurbo FP635 [11] as reporter DNA) of R9-GFP-H6-DNA  
471 polyplexes formed at pH 5.8. GFP-H6 is shown as a control, non-binding protein.

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474 **Figure 2.** Microscopic analysis of R9-GFP-H6-DNA polyplexes. A) Left. Spherical-  
475 shaped green fluorescent signal in HeLa cells exposed for 24 hours to R9-GFP-H6-  
476 DNA polyplexes. Right. Spherical-shaped blue labels for the same field, corresponding  
477 to the embedded DNA. B) Left. Rod-shaped green fluorescent signal in HeLa cells  
478 exposed for 24 hours to R9-GFP-H6-DNA polyplexes. Right. The same field, showing  
479 blue fluorescence corresponding to the embedded DNA. C) Isosurface representation  
480 of polyplexes within a 3D volumetric x-y-z data field, showing the inner localization of  
481 the cargo DNA. Magnification increases in the bottom image. D) Superimposition of  
482 TMV nanodisks and a R9-GFP-H6 molecular model of a stable, planar oligomer [43].  
483 Arginines in the TMV coat protein are located in a radial distribution surrounding the  
484 inner hole (shadowed in yellow, inset), in parallel to those of the R9 tail in R9-GFP-H6  
485 monomers. E) TEM analysis of cell-free R9-GFP-H6 nanoparticles. F) R9-GFP-H6  
486 alone internalized into cultured HeLa cells (upon exposure for 24 h) showing the  
487 absence of any associated DNA.

488

489 **Figure 3.** Functional and structural profiling of DNA-loaded nanoparticles. A)  
490 Remaining plasmid DNA after treatment with DNase I, resulting from protection  
491 mediated by protein shells at alternative retardation units. Different modular proteins  
492 were tested as indicated. At the right, the digestion of protein-free DNA is shown under

493 the same conditions. T indicates time of digestion in min. B) Determination of the z-  
494 potential of R9-GFP-H6 nanoparticles, with and without DNA.

495

496 **Figure 4.** Potential intermolecular contacts in R9-GFP-H6 protein oligomers and in R9-  
497 GFP-H6-DNA polyplexes. A) Protein-protein model configurations were obtained by  
498 docking simulations using HADDOCK at neutral pH, assuming a pentameric  
499 composition that is in agreement with experimental size of protein-only particles. The  
500 first model (left) was obtained using R9 residues as active and H6 residues as passive  
501 [43] and it was used for the superimposition depicted in Figure 2 e. The remaining  
502 three models derived from using R9 residues as active and no passive ones. No  
503 significant differences in packing were obtained when performing the docking runs at  
504 pH 5.8, i.e. with doubly-protonated His (not shown). B) Superposition of the 50  
505 solutions with highest score from a (1:1) DNA-protein docking simulation. The structural  
506 fitting is based on the DNA molecule, which is shown in red.

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