

Arthritis Care & Research
Vol. 68, No. 5, May 2016, pp 603–611
DOI 10.1002/acr.22743

© 2016, The Authors. Arthritis Care & Research published by Wiley Periodicals, Inc. on behalf of the American College of Rheumatology. This is an open access article under the terms of the Creative Commons Attribution License, which permits use, distribution and reproduction in any medium, provided the original work is properly cited.

ORIGINAL ARTICLE

Biomechanical Effects of Prefabricated Foot Orthoses and Rocker-Sole Footwear in Individuals With First Metatarsophalangeal Joint Osteoarthritis

HYLTON B. MENZ,¹ MARIA AUHL,¹ JADE M. TAN,¹ PAZIT LEVINGER,² EDWARD RODDY,³ AND SHANNON E. MUNTEANU¹

Objective. To evaluate the effects of prefabricated foot orthoses and rocker-sole footwear on spatiotemporal parameters, hip and knee kinematics, and plantar pressures in people with first metatarsophalangeal (MTP) joint osteoarthritis (OA).

Methods. A total of 102 people with first MTP joint OA were randomly allocated to receive prefabricated foot orthoses or rocker-sole footwear. The immediate biomechanical effects of the interventions (compared to usual footwear) were examined using a wearable sensor motion analysis system and an in-shoe plantar pressure measurement system.

Results. Spatiotemporal/kinematic and plantar pressure data were available from 88 and 87 participants, respectively. The orthoses had minimal effect on spatiotemporal or kinematic parameters, while the rocker-sole footwear resulted in reduced cadence, percentage of the gait cycle spent in stance phase, and sagittal plane hip range of motion. The orthoses increased peak pressure under the midfoot and lesser toes. Both interventions significantly reduced peak pressure under the first MTP joint, and the rocker-sole shoes also reduced peak pressure under the second through fifth MTP joints and heel. When the effects of the orthoses and rocker-sole shoes were directly compared, there was no difference in peak pressure under the hallux, first MTP joint, or heel; however, the rocker-sole shoes exhibited lower peak pressure under the lesser toes, second through fifth MTP joints, and midfoot.

Conclusion. Prefabricated foot orthoses and rocker-sole footwear are effective at reducing peak pressure under the first MTP joint in people with first MTP joint OA, but achieve this through different mechanisms. Further research is required to determine whether these biomechanical changes result in improvements in symptoms.

INTRODUCTION

Osteoarthritis (OA) is the most common musculoskeletal disorder in the world, affecting 10% of men and 13% of women age >60 years (1). Although the knee is the most

commonly affected lower extremity region, foot involvement is also common. The most commonly affected region of the foot is the first metatarsophalangeal (MTP) joint, with radiographic changes evident in up to 35% of people age >35 years (2). The population prevalence of symptomatic radiographic first MTP joint OA (i.e., both radiographic changes and symptoms) in people age >50 years has recently been estimated as 7.8% (3). First MTP joint

ACTRN: 12613001245785.

Supported by the National Health and Medical Research Council (1049085), Yodgee Footwear (provided footwear at reduced cost), Vasyli Medical (provided prefabricated foot orthoses at reduced cost), and Southern Cross Medical Imaging (provided imaging at reduced cost). Dr. Menz is a National Health and Medical Research Council Senior Research Fellow (1020925) and received funding from the National Health and Medical Research Council of Australia during the course of the study.

¹Hylton B. Menz, PhD, Maria Auhl, PhD, Jade M. Tan, PhD, Shannon E. Munteanu, PhD: La Trobe University, Bundoora, Victoria, Australia; ²Pazit Levinger, PhD: La Trobe University,

Bundoora, Victoria, Australia, and Victoria University, Melbourne, Victoria, Australia; ³Edward Roddy, MBBS, MRCP, DM, FRCP: Keele University, Staffordshire, UK.

Address correspondence to Hylton B. Menz, PhD, School of Allied Health, La Trobe University, Bundoora, Victoria 3086, Australia. E-mail: h.menz@latrobe.edu.au.

Submitted for publication July 6, 2015; accepted in revised form September 22, 2015.

Significance & Innovations

- This is the first study to compare the biomechanical effects of foot orthoses and rocker-sole shoes in people with first metatarsophalangeal (MTP) joint osteoarthritis.
- Both interventions were similarly effective at reducing pressure under the first MTP joint during gait, but achieved this through different mechanisms.
- Foot orthoses increased pressure under the mid-foot and lesser toes.
- Rocker-sole shoes decreased pressure under the second through the fifth MTP joints.

OA has a detrimental impact on health-related quality of life (4), and 72% of those affected report associated locomotor disability (3).

Structural and biomechanical factors are thought to contribute to the onset, progression, and symptomatic severity of first MTP joint OA. During the propulsive phase of gait, the first MTP joint dorsiflexes to assist in the forward transfer of bodyweight. However, in the presence of an overly long and/or wide first metatarsal or proximal phalanx, the proximal phalanx is unable to dorsally rotate on the first metatarsal head, resulting in joint compression and the development of a dorsal exostosis (5). In clinical practice, first MTP joint OA is often managed with foot orthoses, which are thought to decrease pain associated with this condition by allowing the first metatarsal to achieve sufficient plantarflexion in preparation for propulsion, thereby minimizing joint compression (6). Alternatively, pain relief can be achieved using a footwear modification known as a rocker-sole, in which the sole of the shoe is curved (7). The aim of this modification is to allow the body's center of mass to "roll over" the base of support, reducing the need for first MTP joint dorsiflexion and subsequently decreasing the loads placed on the forefoot and toes.

Evidence pertaining to the proposed mechanism of action of foot orthoses in the treatment of first MTP joint OA is limited to a case series study of 9 participants who reported no change in first MTP joint dorsiflexion when the orthoses were worn (8). Studies of asymptomatic participants have been inconsistent, with 2 studies reporting a decrease in first MTP joint dorsiflexion (with medial wedging [9] and orthoses [10]) and a recent study demonstrating a small increase in the declination angle of the first metatarsal when participants wore an orthosis with material removed from beneath the first MTP joint (11). No studies have been undertaken to assess the biomechanical effects of rocker-sole shoes in participants with first MTP joint OA, although studies in asymptomatic participants indicate a reduction in sagittal plane motion of the forefoot (12) and ankle (12–15), reduced forefoot plantar pressures (15,16), and reduced first MTP joint dorsiflexion (17) when walking compared to usual footwear.

Given the uncertainty regarding the mechanism of action of these 2 treatments, the objective of this study was to evaluate the immediate biomechanical effects of in-

dividualized, prefabricated foot orthoses and rocker-sole shoes in individuals with first MTP joint OA. To do this, we conducted baseline kinematic and in-shoe plantar pressure analyses of participants enrolled in a randomized trial (18) when wearing their usual footwear and their allocated intervention (i.e., orthoses or rocker-sole shoes).

MATERIALS AND METHODS

The data presented in this paper were collected at the baseline assessment of a larger randomized trial (Australian New Zealand Clinical Trials Registry ID: 12613001245785). The La Trobe University Human Ethics Committee provided ethical approval (13-003), and all participants provided written informed consent prior to enrollment. The full trial protocol has been published previously (18).

Design. The study design was a parallel-group, randomized trial comparing 2 interventions: prefabricated foot orthoses (Vasyli Custom, Vasyli Medical) versus commercially available rocker-sole footwear (Masai Barefoot Technology [MBT], Matwa model). Permuted block randomization with random block sizes, stratified by sex, was undertaken using an interactive voice response telephone service provided by the National Health and Medical Research Council Clinical Trials Centre at the University of Sydney, New South Wales, Australia to ensure allocation concealment. Participants were informed that they would receive either the foot orthoses or rocker-sole footwear (i.e., they were not blinded to their group allocation).

Participant recruitment, screening, and eligibility criteria. To be included in the study, participants had to 1) be age ≥ 18 years; 2) report having pain in the first MTP joint on most days for at least 12 weeks; 3) report having pain rated at least 20 mm on a 100-mm visual analog scale; 4) have $< 64^\circ$ of dorsiflexion range of motion (ROM) of the first MTP joint (19); 5) have pain upon palpation of the dorsal aspect of the first MTP joint; 6) be able to walk household distances (> 50 meters) without the aid of a walker, crutches, or cane; 7) be willing to attend the Health Sciences Clinic at La Trobe University (Melbourne, Victoria) on 2 occasions and have their foot radiographed; 8) be willing to not receive additional interventions (such as physical therapy, foot orthoses, shoe modifications, intraarticular injections, or surgery) for first MTP joint pain during the course of the study; and 9) be willing to discontinue taking all medications to relieve pain at their first MTP joint (analgesics and nonsteroidal antiinflammatory medications, except paracetamol up to 4 gm/day) for at least 14 days prior to the baseline assessment and during the study period.

Exclusion criteria for participants in this study were 1) pregnancy; 2) previous surgery on the first MTP joint; 3) significant deformity of the first MTP joint including hallux valgus (grade of 3 or 4, using the Manchester Scale) (20,21); 4) presence of 1 or more conditions within the foot or ankle that could confound pain and functional assessments of the first MTP joint, such as metatarsalgia, plantar fasciitis, predislocation syndrome, Achilles ten-



Figure 1. Prefabricated foot orthoses used in the trial. **Top**, plantar surface of left foot orthosis; **bottom**, dorsal surface of right foot orthosis. Reproduced from ref. 18. Color figure can be viewed in the online issue, which is available at <http://onlinelibrary.wiley.com/journal/doi/10.1002/acr.22743/abstract>.

dinopathy, and degenerative joint disease (other than the first MTP joint); 5) presence of any systemic inflammatory condition, such as inflammatory arthritis, rheumatoid arthritis, ankylosing spondylitis, psoriatic arthritis, reactive arthritis, septic arthritis, acute pseudogout, gout, or any other connective tissue disease; 6) any medical condition that, in the opinion of the investigators, made the participant unsuitable for inclusion (e.g., severe progressive chronic disease, malignancy, clinically important pain in a part of the musculoskeletal system other than the first MTP joint, or fibromyalgia); 7) cognitive impairment (defined as a score of <7 on the Short Portable Mental Status Questionnaire) (22); 8) intraarticular injections into the first MTP joint in the previous 6 months; 9) currently wearing contoured foot orthoses (although flat insoles were permitted); 10) currently wearing specialized footwear (footwear that has been custom-made or “prescribed” by a health care practitioner); 11) currently wearing shoes that would not be able to accommodate a foot orthosis; or 12) older adults with a history of recurrent falls (defined as 2 or more falls in the previous 12 months), as there is some evidence that rocker-sole shoes may have short-term detrimental effects on balance (23).

Participants were recruited by 1) radio advertisements; 2) advertisements placed in local newspapers, magazines, and social media; 3) posters placed at health care facilities, gymnasiums, senior citizens’ centers, fun runs, and markets; and 4) mail-out advertisements to patients attending the La Trobe University Health Sciences clinic and to local podiatry clinics. Baseline testing was performed between February and October 2014.

Clinical and radiographic assessment. At baseline, participants underwent a clinical assessment, including measurements of height, weight, and body mass index; foot posture (using the Foot Posture Index [FPI]) (24); pas-

sive, non-weight-bearing dorsiflexion ROM at the first MTP joint using a flexible, plastic hand-held goniometer (25); and observation to determine the presence or absence of pain on palpation, a dorsal exostosis, joint effusion, pain during motion, a hard-end feel when the joint was fully dorsiflexed, and crepitus during movement. The reliability of these assessments has previously been documented (19). Footwear was assessed using the Footwear Assessment Form (26).

The presence or absence of radiographic first MTP joint OA was determined using a radiographic atlas developed by Menz et al (27). The atlas incorporates weight-bearing dorsoplantar and lateral radiographs to document the presence of OA based on observations of osteophytes and joint space narrowing. Osteophytes were recorded as absent (score 0), small (score 1), moderate (score 2), or severe (score 3). Joint space narrowing was recorded as none (score 0), definite (score 1), severe (score 2), or joint fusion (score 3). The atlas has been shown to have good to excellent intra- and interrater reliability for grading first MTP joint OA ($\kappa = 0.64\text{--}0.95$) (27).

Interventions. The prefabricated foot orthoses group received a pair of foot orthoses (Vasyli Custom Medium Density) that were modified using a similar approach to that described by Welsh et al (8). All orthoses were full length, but were modified by adding a cut-out section beneath the first metatarsal and trimming the distal edge to the level of the second to fifth toe sulci (Figure 1). In participants with pronated feet (defined as an FPI score of >7) (28), full-length 4-degree medial (varus) wedges were applied to the underside of the foot orthoses until there was a reduction in the FPI score of at least 2 points (8). The wedge was gradually bevelled so that it extended to the proximal margin of the cut-out section beneath the first metatarsal. This occurred for 2 participants.

The rocker-sole footwear group was provided with a pair of appropriately sized rocker-sole shoes (MBT, Matwa model). This shoe is characterized by a rounded sole in the anteroposterior direction and a soft cushioned heel (Figure 2). Across the full size range, the radius of curvature of the MBT shoe is on average 33 cm overall, 18 cm at the forefoot, 43 cm at the midfoot, and 11 cm at the heel (29). After commencing the study, the MBT shoe we used (the “Mahuta” model) was discontinued by the company and replaced with the “Matwa” model, resulting in 4 participants receiving



Figure 2. Matwa model footwear (Masai Barefoot Technology). Reproduced from ref. 18. Color figure can be viewed in the online issue, which is available at <http://onlinelibrary.wiley.com/journal/doi/10.1002/acr.22743/abstract>.

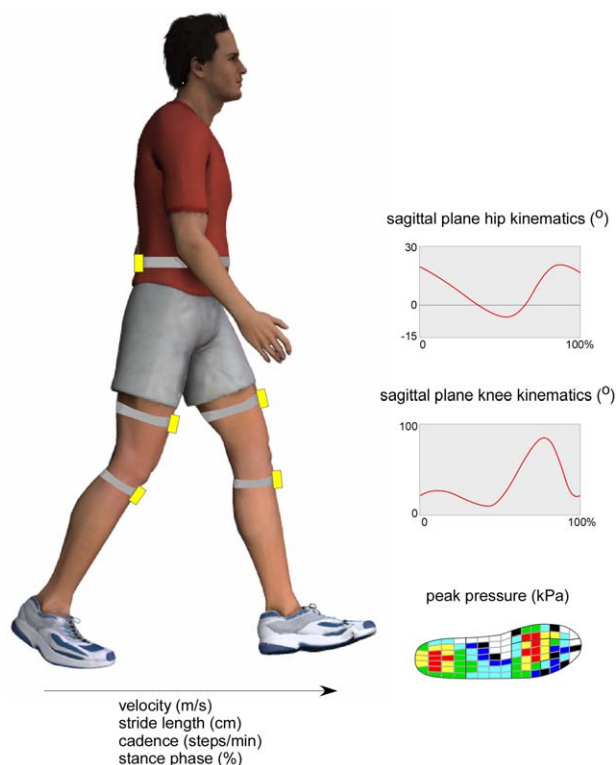


Figure 3. Gait analysis system. Color figure can be viewed in the online issue, which is available at <http://onlinelibrary.wiley.com/journal/doi/10.1002/acr.22743/abstract>.

the Mahuta and 42 receiving the Matwa. However, both models had the same sole curvature and only differed slightly in relation to the aesthetics of the upper.

Gait analysis. Both groups underwent the same biomechanical assessment. However, for the prefabricated foot orthoses group, comparisons were made when wearing their own shoes (with and without the prefabricated orthoses), while for the rocker-sole shoe group, comparisons were made between their own shoes and the rocker-sole shoes. The order of testing was randomized. After a familiarization period of walking 250 meters, participants completed 4 walking trials for each footwear condition over an 8-meter distance. To exclude the effect of acceleration and deceleration steps, only the middle 4 steps from each trial were included for analysis. An average recording was determined from 16 steps for each condition. Walking speed was intentionally not controlled for, in order to provide insights into how participants would function under real-world conditions.

Spatiotemporal parameters and sagittal plane peak-to-trough ROM of the hip and knee joints during gait were recorded using a wireless, wearable sensor motion analysis system (LEGSys, Biosensics). This system consists of accelerometers and gyroscopes attached with Velcro straps to each lower leg and thigh (Figure 3). The method for calculation of the spatiotemporal parameters of gait is described in detail elsewhere (30). To summarize, the gait phases are determined from the precise events of heel-strike (initial foot contact) until toe-off (terminal foot con-

tact). These events are extracted from gyroscopes attached to each shank through a local minimal peak detection scheme. Based on each participant's height and using a biomechanical model, spatial parameters (i.e., stride length and stride velocity) and kinematics (hip and knee) are estimated by integration of the angular rate of rotation of the thigh and shank relative to the waist sensor. Gait analysis with this system has been validated in healthy young controls (30) and older people (31) and has been shown to exhibit acceptable reliability (32).

Peak plantar pressure under the hallux, lesser toes, first MTP joint, second to fifth MTP joints, midfoot, and heel were measured with the in-shoe Pedar system (Novel GmbH), a reliable, valid, and accurate measure of in-shoe pressure (33–35). The Pedar insoles are approximately 2-mm thick and consist of 99 capacitive pressure sensors arranged in grid alignment. Plantar pressure data were sampled at a frequency of 50 Hz.

Statistical analysis. Statistical analysis was undertaken using SPSS, version 22.0. The most symptomatic foot was selected as the index foot for all analyses, or in the case of equivalent symptoms in both feet, the right foot was selected. All data were explored for normality using the skewness statistic (-1 to 1). To evaluate the effects of the interventions (i.e., prefabricated orthoses and rocker-sole shoes) compared to participants' own footwear, a series of within-group, paired *t*-tests were conducted. To compare the effects of prefabricated orthoses and rocker-sole shoes, between-group analyses of covariance were conducted with the intervention group and participants' own footwear scores entered as independent variables (36). The effect size for within-group comparisons was calculated using Cohen's *d*, and the following interpretation of effect size was used: negligible (<0.15), small (≥ 0.15 to <0.40), medium (≥ 0.40 to <0.75), large (≥ 0.75 to <1.10), and very large (≥ 1.10) (37). Adjusted mean differences and 95% confidence intervals were calculated for between-group comparisons.

RESULTS

Participants. A total of 102 participants were randomized into the study. Five withdrew prior to the baseline assessment, leaving 97 who underwent gait analysis. Characteristics of these participants are reported in Table 1. Due to technical issues with data collection, spatiotemporal/kinematic data were missing from 9 participants, and plantar pressure data were missing from 7 participants. Furthermore, upon initial screening of the data, it was noted that there were 3 significant outliers for peak pressure under the first MTP joint, where extremely high peak pressures were registered for 1 or 2 individual sensors on the most medial edge of the insole. Because the pressure readings obtained from these sensors were unilateral and markedly higher than adjacent sensors, it was concluded that they were due to the Pedar insole being folded or compressed against the medial upper of the shoe. For this reason, first MTP joint peak pressure data from these 3 participants were excluded from the analysis. Therefore, complete spatiotemporal/

Table 1. Participant characteristics*		
	Orthoses group (n = 51)	Rocker-sole group (n = 46)
Demographics and anthropometrics		
Age, years	57.0 ± 11.2	56.5 ± 11.1
Female, no. (%)	28 (54.9)	28 (60.9)
Height, cm	166.2 ± 8.8	166.3 ± 8.3
Weight, kg	80.7 ± 15.0	78.5 ± 13.3
Body mass index, kg/m ²	29.2 ± 4.8	28.4 ± 4.5
Clinical features		
Pain duration, median (range) months	36 (4–360)	30 (6–420)
Foot Posture Index, mean ± SD (range)	3.0 ± 2.5 (–2 to 11)	3.4 ± 2.2 (–2 to 10)
First MTP joint ROM, degrees	39.8 ± 12.7	40.5 ± 13.0
Pain on palpation, no. (%)	51 (100.0)	46 (100)
Palpable dorsal exostosis, no. (%)	49 (96.1)	45 (97.8)
Joint effusion, no. (%)	17 (34.0)	16 (34.8)
Pain on motion of first MTP joint, no. (%)	49 (96.1)	41 (91.1)
Hard-end feel when dorsiflexed, no. (%)	46 (90.2)	39 (84.8)
Crepitus, no. (%)	35 (68.6)	30 (65.2)
Radiographic features, no. (%)†		
Dorsal osteophytes	48 (96.0)	38 (84.0)
Dorsal joint space narrowing	43 (86.0)	36 (80.0)
Lateral osteophytes	43 (86.0)	35 (77.8)
Lateral joint space narrowing	42 (84.0)	38 (84.4)
Radiographic first MTP joint OA‡	38 (79.2)	30 (66.7)
Footwear characteristics		
Walking/athletic/Oxford shoe, no. (%)	32 (62.7)	26 (56.5)
Mary Jane/court shoe/boot, no. (%)	9 (17.6)	13 (28.2)
Sandal/slipper/moccasin, no. (%)	10 (19.6)	7 (15.2)
Heel height, mm	23.8 ± 7.9	22.4 ± 10.5
Forefoot height, mm	12.2 ± 5.1	12.2 ± 5.7
Sole flexion point, no. (%)		
At level of MTP joints	35 (68.6)	28 (60.9)
Proximal to MTP joints	10 (19.6)	12 (26.1)
Distal to MTP joints	6 (11.8)	6 (13.0)
* Values are the mean ± SD unless indicated otherwise. MTP = metatarsophalangeal; ROM = range of motion; OA = osteoarthritis.		
† Score >0 using atlas in ref. 27.		
‡ At least one score of 2 for osteophytes or joint space narrowing from either view, using case definition from atlas in ref. 27.		

kinematic and plantar pressure data were available from 88 and 87 participants, respectively.

Spatiotemporal and kinematic data. Spatiotemporal and kinematic data are shown in Table 2. Compared to participants' own footwear, the orthoses had minimal effects on spatiotemporal or kinematic parameters, with a reduction in velocity (Cohen's $d = 0.14$; negligible effect) and knee ROM ($d = 0.36$; small effect) observed, while the rocker-sole shoes resulted in reduced cadence ($d = 0.26$; small effect), percentage of the gait cycle spent in stance phase ($d = 0.44$; medium effect), and reduced sagittal plane hip ROM ($d = 0.44$; medium effect). Between-group comparisons indicated that the percentage of the gait cycle spent in stance phase and sagittal plane hip ROM was lower in the rocker-sole shoe group compared to the orthoses group.

Plantar pressure data. Typical examples of peak pressure recordings are shown in Figure 4, and complete peak

plantar pressure data are shown in Table 2. Compared to participants' own footwear, the orthoses increased peak pressure under the lesser toes ($d = 0.59$; medium effect) and midfoot ($d = 0.45$; medium effect), and decreased peak pressure under the first MTP joint ($d = 0.55$; medium effect) and heel ($d = 0.72$; medium effect), while the rocker-sole shoes decreased peak pressure under the first MTP joint ($d = 0.44$; medium effect), second to fifth MTP joints ($d = 0.92$; large effect), and heel ($d = 0.91$; large effect). Between-group comparisons indicated that the peak pressure under the lesser toes, second to fifth MTP joints, and midfoot was lower in the rocker-sole shoes compared to the orthoses, but there was no difference in peak pressure under the first MTP joint.

DISCUSSION

The objective of this study was to compare the immediate biomechanical effects of prefabricated foot orthoses and rocker-sole footwear in people with first MTP joint OA. Our findings

Table 2. Effects of orthoses and rocker-sole shoes on spatiotemporal/kinematic and plantar pressure parameters*

	Orthoses group†			Rocker-sole group†			Between-group comparisons		
	Own footwear	Own footwear + orthoses	P	Own footwear	Rocker-sole footwear	P	Adjusted mean difference (95% CI)‡	P	P
Spatiotemporal/kinematic									
Velocity (minutes/second)	1.06 ± 0.15	1.04 ± 0.14	0.039	1.04 ± 0.13	1.00 ± 0.14	0.075	-0.02 (-0.06, 0.02)	0.374	
Stride length (meters)	1.16 ± 0.15	1.15 ± 0.14	0.280	1.11 ± 0.13	1.10 ± 0.14	0.408	-0.02 (-0.06, 0.02)	0.396	
Cadence (steps/minute)	109.72 ± 8.09	108.46 ± 8.42	0.055	112.02 ± 8.65	109.85 ± 8.54	0.015	-0.53 (-2.58, 1.53)	0.610	
Stance phase (%)	59.69 ± 2.03	59.90 ± 2.14	0.479	59.66 ± 1.77	58.84 ± 2.03	0.021	-1.04 (-1.84, -0.25)	0.010	
Sagittal knee ROM	60.89 ± 8.30	57.94 ± 8.31	0.027	59.75 ± 11.69	59.06 ± 9.71	0.576	1.76 (-1.27, 4.78)	0.252	
Sagittal hip ROM	47.93 ± 5.03	47.61 ± 5.95	0.587	46.44 ± 4.90	44.46 ± 4.26	0.006	-2.11 (-3.80, -0.42)	0.015	
Plantar pressure (kPa)									
Hallux	231.22 ± 92.94	243.11 ± 98.95	0.120	244.11 ± 92.47	252.68 ± 112.14	0.533	-1.42 (-31.49, 28.65)	0.925	
Lesser toes	116.94 ± 39.40	139.50 ± 37.51	<0.001	131.90 ± 56.04	126.25 ± 37.92	0.502	-19.21 (-33.31, -5.10)	0.008	
First MTP joint	161.99 ± 54.44	132.95 ± 51.98	<0.001	166.06 ± 50.44	146.19 ± 39.48	0.002	10.56 (-3.07, 24.20)	0.127	
Second through fifth MTP joints	223.67 ± 57.15	236.89 ± 63.26	0.056	223.45 ± 60.83	173.69 ± 48.26	<0.001	-63.08 (-82.96, -43.20)	<0.001	
Midfoot	95.89 ± 32.51	109.61 ± 29.13	<0.001	86.43 ± 29.36	90.54 ± 23.78	0.356	-14.21 (-23.49, -4.92)	0.003	
Heel	226.78 ± 69.71	187.67 ± 34.42	<0.001	213.51 ± 49.05	174.11 ± 37.36	<0.001	-10.01 (-23.38, 3.81)	0.153	

* Values are the mean ± SD. 95% CI = 95% confidence interval; ROM = range of motion; MTP = metatarsophalangeal.

† Within-group comparisons.

‡ Mean difference between interventions, adjusted for own footwear (control) condition.

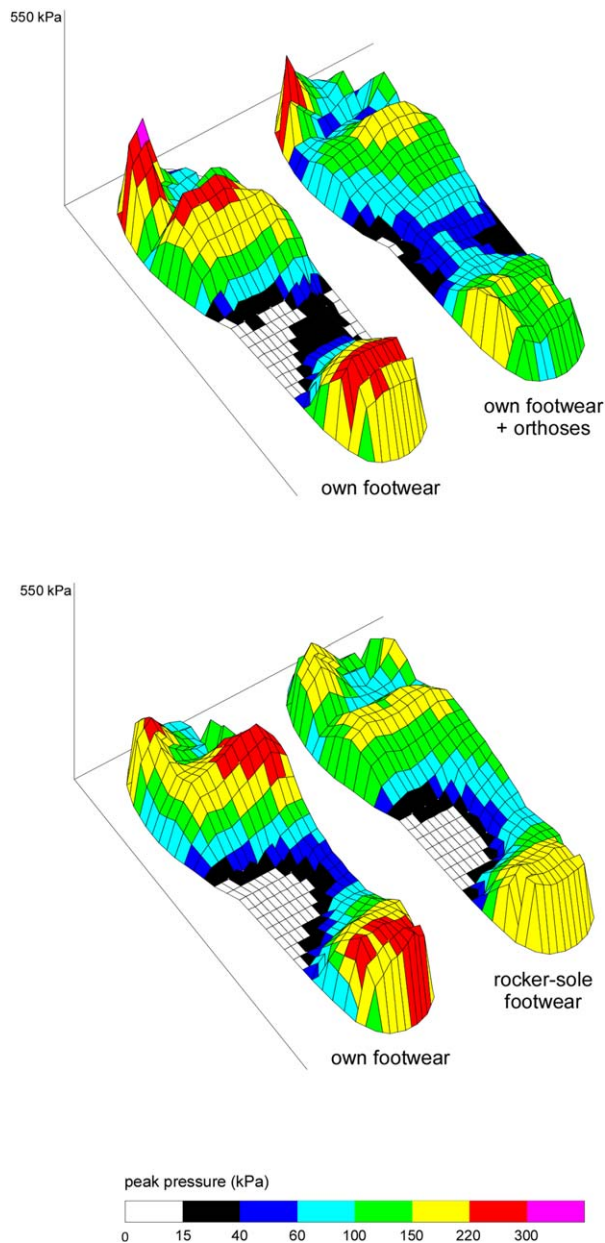


Figure 4. Typical plantar pressure recordings taken from a participant allocated to the orthoses group (**top**) and to the rocker-sole footwear group (**bottom**). Images represent the mean of 8 steps for the index (**right**) foot. Note the reduced peak pressure under the forefoot and heel, and increased pressure under the midfoot associated with both interventions compared to the participant's own footwear.

indicate that both interventions were effective at reducing peak pressure beneath the first MTP joint, which may be one of the mechanisms responsible for their apparent beneficial effects in the treatment of OA affecting this joint. However, they appear to achieve this through different mechanisms. The prefabricated orthoses had minimal effect on spatiotemporal or kinematic parameters, while the rocker-sole footwear resulted in reduced cadence, percentage of the gait cycle spent in stance phase, and sagittal plane hip ROM. Plantar pressure assessment also revealed that the prefabricated foot orthoses produced an increase in peak pressure under the

lesser toes and midfoot and a decrease under the heel, while the rocker-sole shoes were associated with decreased peak pressure under the second to fifth MTP joints and heel.

The prefabricated orthoses in this study were modified by the addition of a cut-out section beneath the first metatarsal, as described by Welsh et al (8). The rationale behind this approach is to facilitate first ray plantarflexion, thereby allowing the proximal phalanx to dorsiflex on the first metatarsal head and minimize joint compression during propulsion (6). However, the gait analysis component of the study by Welsh et al found no differences in first MTP joint dorsiflexion when orthoses were worn, despite participants reporting a reduction in symptoms. Our in-shoe plantar pressure data suggest that orthoses may instead achieve their apparent beneficial effects by redistributing load away from the first MTP joint, possibly by shifting it toward the medial longitudinal arch during midstance and toward the lesser toes during propulsion. Increased midfoot load appears to be a consistent and predictable effect of wearing orthoses, which contour the arch (38,39). However, the shift in load toward the lateral toes observed in this study is a novel finding and may be specific to the style of orthosis we used (incorporating a cut-out section beneath the first metatarsal) and/or the condition being studied (first MTP joint OA).

The biomechanical effects of rocker-sole footwear have been examined in several studies, but none have specifically examined individuals with first MTP joint OA. Our observation of reduced hip joint ROM is consistent with previous investigations using a variety of rocker-sole designs (13,40–42), and has primarily been attributed to the adoption of a shorter stride length. In our study, stride length was not significantly altered when wearing the rocker-sole shoes. However, there was a reduction in cadence and a trend ($P = 0.08$) toward reduced velocity, both of which may reflect the adoption of a “cautious” gait pattern that has been shown to result in reduced sagittal plane hip motion during gait (43). The combination of a posterior heel rocker, shock-absorbing heel, and anterior rocker in the MBT shoe may also have a direct influence on hip motion, as less hip flexion may be required for the foot to clear the ground in preparation for initial heel contact (40), the decrease in vertical ground reaction force during contact phase (42) may reduce the internal hip extensor moment, and the relatively “passive” push-off may require less hip extension during propulsion.

Consistent with several previous studies of a range of rocker-sole shoes (44–46), the in-shoe plantar pressure evaluation revealed a significant reduction in forefoot peak pressure. This finding, combined with our observation of a smaller relative proportion of the gait cycle spent in stance phase, suggests that this style of footwear facilitates forward momentum by enabling the body's center of mass to passively “roll over” the base of support, rather than achieving propulsion through ankle power generation at push-off. Indeed, studies of gait kinetics when wearing rocker-sole footwear have reported reductions in peak internal ankle plantarflexor moment (42) and plantarflexor power generation (41) during late stance phase, which is indicative of reduced concentric function of the triceps surae. Given that a reduction in forefoot pressures

has been shown to be associated with pain relief in people with forefoot pain (47), it is possible that such a change may also be therapeutically beneficial in people with symptomatic first MTP joint OA by offloading the painful area and reducing joint compression.

The findings of this study need to be considered in the context of several design limitations. First, it was not possible to blind participants to their intervention allocation. Second, the observed changes are immediate effects only, as all gait assessments were performed at the baseline assessment. Although we allowed participants a familiarization period to adapt to their orthoses and footwear, we acknowledge that the effects of the interventions are likely to change over time. Indeed, Stöggl et al (48) have shown that the gait variability induced by MBT shoes significantly reduces after 10 weeks of daily wear, suggesting that some degree of habituation occurs. Third, our gait analysis technique did not allow for in-shoe assessment of first MTP joint kinematics, as this requires the permanent modification of the upper of the shoe to enable placement of reflective markers or electromagnetic sensors. This approach can compromise the structural integrity of the shoe (49) and is clearly not feasible in the context of a prospective trial where participants are expected to wear the shoes during daily activities over several weeks. Fourth, the wearable sensor motion analysis system we used is restricted to sagittal plane evaluation of the knee and hip. Finally, an inherent limitation of commercially available in-shoe plantar pressure measurement systems such as the Pedar is that they only measure force perpendicular to the sensor surface. Therefore, the accuracy of measurements made along curved surfaces (such as the medial arch of foot orthoses) may be limited.

In summary, this study has shown that prefabricated foot orthoses and rocker-sole footwear are effective at reducing peak pressure under the first MTP joint in people with first MTP joint OA; however, they appear to achieve this through different mechanisms. The planned 12-week followup will determine whether these interventions are acceptable to participants and are effective at reducing joint pain.

ACKNOWLEDGMENTS

The authors wish to thank Gary Yodgee (Yodgee Footwear), and Matt Barkley and Craig Truscott (Vasyli Medical).

AUTHOR CONTRIBUTIONS

All authors were involved in drafting the article or revising it critically for important intellectual content, and all authors approved the final version to be submitted for publication. Dr. Menz had full access to all of the data in the study and takes responsibility for the integrity of the data and the accuracy of the data analysis.

Study conception and design. Menz, Levinger, Roddy, Munteanu.
Acquisition of data. Menz, Auhl, Tan, Munteanu.
Analysis and interpretation of data. Menz, Auhl, Tan, Levinger, Roddy, Munteanu.

REFERENCES

1. World Health Organisation. The burden of musculoskeletal conditions at the start of the new millenium: report of a WHO scientific group. WHO Technical Report Series No. 919. 2003. URL: http://apps.who.int/iris/bitstream/10665/42721/1/WHO_TRS_919.pdf.
2. Trivedi B, Marshall M, Belcher J, Roddy E. A systematic review of radiographic definitions of foot osteoarthritis in population-based studies. *Osteoarthritis Cartilage* 2010;18:1027–35.
3. Roddy E, Thomas MJ, Marshall M, Rathod T, Myers H, Menz HB, et al. The population prevalence of symptomatic radiographic foot osteoarthritis in community-dwelling older adults: the Clinical Assessment Study of the Foot. *Ann Rheum Dis* 2015;74:156–63.
4. Bergin SM, Munteanu SE, Zammit GV, Nikolopoulos N, Menz HB. Impact of first metatarsophalangeal joint osteoarthritis on health-related quality of life. *Arthritis Care Res (Hoboken)* 2012;64:1691–8.
5. Zammit GV, Menz HB, Munteanu SE. Structural factors associated with hallux limitus/rigidus: a systematic review of case control studies. *J Orthop Sports Phys Ther* 2009;39:733–42.
6. Rosenbloom KB. Pathology-designed custom molded foot orthoses. *Clin Podiatr Med Surg* 2011;28:171–87.
7. Hutchins S, Bowker P, Geary N, Richards J. The biomechanics and clinical efficacy of footwear adapted with rocker profiles: evidence in the literature. *Foot* 2009;19:165–70.
8. Welsh BJ, Redmond AC, Chockalingam N, Keenan AM. A case-series study to explore the efficacy of foot orthoses in treating first metatarsophalangeal joint pain. *J Foot Ankle Res* 2010;3:17.
9. Smith C, Spooner SK, Fletton JA. The effect of 5-degree valgus and varus rearfoot wedging on peak hallux dorsiflexion during gait. *J Am Podiatr Med Assoc* 2004;94:558–64.
10. Michaud TC, Nawoczenski DA. The influence of two different types of foot orthoses on first metatarsophalangeal joint kinematics during gait in a single subject. *J Manipulative Physiol Ther* 2006;29:60–5.
11. Becerro de Bengoa Vallejo R, Gomez RS, Losa Iglesias ME. Clinical improvement in functional hallux limitus using a cut-out orthosis. *Prosth Orth Int* 2014. E-pub ahead of print.
12. Wu WL, Rosenbaum D, Su FC. The effects of rocker sole and SACH heel on kinematics in gait. *Med Eng Phys* 2004;26:639–46.
13. Romkes J, Rudmann C, Brunner R. Changes in gait and EMG when walking with the Masai Barefoot Technique. *Clin Biomech* 2006;21:75–81.
14. Landry SC, Nigg BM, Tecante KE. Walking in an unstable Masai Barefoot Technology (MBT) shoe introduces kinematic and kinetic changes at the hip, knee and ankle before and after a 6-week accommodation period: a comprehensive analysis using principal components analysis (PCA). *Footwear Sci* 2012;4:101–14.
15. Forghany S, Nester CJ, Richards B, Hatton AL, Liu A. Roll-over footwear affects lower limb biomechanics during walking. *Gait Posture* 2014;39:205–12.
16. Stewart L, Gibson JN, Thomson CE. In-shoe plantar pressure distribution in “unstable” (MBT) shoes and flat-bottomed training shoes: a comparative study. *Gait Posture* 2007;25:648–51.
17. Lin SC, Chen C, Tang S, Wong A, Hsieh JH. Changes in windlass effect in response to different shoe and insole designs during walking. *Gait Posture* 2013;37:235–41.
18. Menz HB, Levinger P, Tan JM, Auhl M, Roddy E, Munteanu SE. Rocker-sole footwear versus prefabricated foot orthoses for the treatment of pain associated with first metatarsophalangeal joint osteoarthritis: study protocol for a randomised trial. *BMC Musculoskelet Disord* 2014;15:86.
19. Zammit GV, Munteanu SE, Menz HB. Development of a diagnostic rule for identifying radiographic osteoarthritis in people with first metatarsophalangeal joint pain. *Osteoarthritis Cartilage* 2011;19:939–45.
20. Garrow AP, Papageorgiou A, Silman AJ, Thomas E, Jayson MI, Macfarlane GJ. The grading of hallux valgus: the Manchester Scale. *J Am Podiatr Med Assoc* 2001;91:74–8.

21. Menz HB, Munteanu SE. Radiographic validation of the Manchester Scale for the classification of hallux valgus deformity. *Rheumatology (Oxford)* 2005;44:1061–6.
22. Pfeiffer E. A short portable mental status questionnaire for the assessment of organic brain deficit in elderly patients. *J Am Geriatr Soc* 1975;23:433–41.
23. Albright BC, Woodhull-Smith WM. Rocker bottom soles alter the postural response to backward translation during stance. *Gait Posture* 2009;30:45–9.
24. Redmond AC, Crosbie J, Ouvrier RA. Development and validation of a novel rating system for scoring standing foot posture: the Foot Posture Index. *Clin Biomech* 2006;21:89–98.
25. Buell T, Green DR, Risser J. Measurement of the first metatarsophalangeal joint range of motion. *J Am Podiatr Med Assoc* 1988;78:439–48.
26. Barton CJ, Bonanno D, Menz HB. Development and evaluation of a tool for the assessment of footwear characteristics. *J Foot Ankle Res* 2009;2:10.
27. Menz HB, Munteanu SE, Landorf KB, Zammit GV, Cicuttini FM. Radiographic classification of osteoarthritis in commonly affected joints of the foot. *Osteoarthritis Cartilage* 2007;15:1333–8.
28. Redmond AC, Crane YZ, Menz HB. Normative values for the Foot Posture Index. *J Foot Ankle Res* 2008;1:6.
29. Forghany S, Nester CJ, Richards B. The effect of rollover footwear on the rollover function of walking. *J Foot Ankle Res* 2013;6:24.
30. Aminian K, Najafi B, Bula C, Leyvraz PF, Robert P. Spatio-temporal parameters of gait measured by an ambulatory system using miniature gyroscopes. *J Biomech* 2002;35:689–99.
31. Najafi B, Helbostad JL, Moe-Nilssen R, Zijlstra W, Aminian K. Does walking strategy in older people change as a function of walking distance? *Gait Posture* 2009;29:261–6.
32. Najafi B, Khan T, Wrobel J. Laboratory in a box: wearable sensors and its advantages for gait analysis. *Conf Proc IEEE Eng Med Biol Soc* 2011;2011:6507–10.
33. Boyd LA, Bontrager EL, Mulroy SJ, Perry J. The reliability and validity of the novel Pedar system of in-shoe pressure measurement during free ambulation. *Gait Posture* 1997;5:165.
34. Murphy DF, Beynon BD, Michelson JD, Vacek PM. Efficacy of plantar loading parameters during gait in terms of reliability, variability, effect of gender and relationship between contact area and plantar pressure. *Foot Ankle Int* 2005;26:171–9.
35. Putti AB, Arnold GP, Cochrane L, Abboud RJ. The Pedar in-shoe system: repeatability and normal pressure values. *Gait Posture* 2007;25:401–5.
36. Vickers AJ, Altman DG. Statistics notes: analysing controlled trials with baseline and follow up measurements. *BMJ* 2001;323:1123–4.
37. Thalheimer W, Cook S. How to calculate effect sizes from published research articles: a simplified methodology. 2002. URL: http://work-learning.com/effect_sizes.htm.
38. Cronkwright DG, Spink MJ, Landorf KB, Menz HB. Evaluation of the pressure-redistributing properties of prefabricated foot orthoses in older people after at least 12 months of wear. *Gait Posture* 2011;34:553–7.
39. Bonanno DR, Landorf KB, Menz HB. Pressure-relieving properties of various shoe inserts in older people with plantar heel pain. *Gait Posture* 2011;33:385–9.
40. Myers KA, Long JT, Klein JP, Wertsch JJ, Janisse D, Harris GF. Biomechanical implications of the negative heel rocker sole shoe: gait kinematics and kinetics. *Gait Posture* 2006;24:323–30.
41. Buchecker M, Lindinger S, Pfusterschmied J, Muller E. Effects of age on lower extremity joint kinematics and kinetics during level walking with Masai barefoot technology shoes. *Eur J Phys Rehabil Med* 2013;49:675–86.
42. Taniguchi M, Tateuchi H, Takeoka T, Ichihashi N. Kinematic and kinetic characteristics of Masai Barefoot Technology footwear. *Gait Posture* 2012;35:567–72.
43. Crowinshield RD, Brand RA, Johnston RC. The effects of walking velocity and age on hip kinematics and kinetics. *Clin Orthop Relat Res* 1978;132:140–4.
44. Nawoczenski DA, Birke JA, Coleman WC. Effect of a rocker sole design on plantar forefoot pressures. *J Am Podiatr Med Assoc* 1988;78:455–60.
45. Schaff PS, Cavanagh PR. Shoes for the insensitive foot: the effect of a “rocker bottom” shoe modification on plantar pressure distribution. *Foot Ankle* 1990;11:129–40.
46. Brown D, Wertsch JJ, Harris GF, Klein J, Janisse D. Effect of rocker soles on plantar pressures. *Arch Phys Med Rehabil* 2004;85:81–6.
47. Kang JH, Chen MD, Chen SC, Hsi WL. Correlations between subjective treatment responses and plantar pressure parameters of metatarsal pad treatment in metatarsalgia patients: a prospective study. *BMC Musculoskelet Disord* 2006;7:95.
48. Stoggl T, Haudum A, Birklbauer J, Murrer M, Muller E. Short and long term adaptation of variability during walking using unstable (MBT) shoes. *Clin Biomech* 2010;25:816–22.
49. Shultz R, Jenkyn T. Determining the maximum diameter for holes in the shoe without compromising shoe integrity when using a multi-segment foot model. *Med Eng Phys* 2012;34:118–22.