

1 2	Influence of Cold Water Immersion on Limb Blood Flow after Resistance Exercise
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48 ABSTRACT

49 This study determined the influence of cold (8°C) and cool (22°C) water immersion 50 on lower limb and cutaneous blood flow following resistance exercise. Twelve males 51 completed 4-sets of 10-repetition maximum squat exercise and were then immersed, 52 semi-reclined, into 8°C or 22°C water for 10-min, or rested in a seated position 53 (control) in a randomized order on different days. Rectal and thigh skin temperature, 54 muscle temperature, thigh and calf skin blood flow and superficial femoral artery 55 blood flow were measured before and after immersion. Indices of vascular 56 conductance were calculated (flux and blood flow/mean arterial pressure). The colder 57 water reduced thigh skin temperature and deep muscle temperature to the greatest 58 extent (P < 0.001). Reductions in rectal temperature were similar ($0.2^{\circ}C-0.4^{\circ}C$) in all 59 three trials (P = 0.69). Femoral artery conductance was similar after immersion in 60 both cooling conditions, with both conditions significantly lower (55%) than the control post-immersion (P < 0.01). Similarly, there was greater thigh and calf 61 62 cutaneous vasoconstriction (40-50%) after immersion in both cooling conditions, 63 relative to the control (P < 0.01), with no difference between cooling conditions. These findings suggest that cold and cool water similarly reduce femoral artery and 64 65 cutaneous blood flow responses but not muscle temperature following resistance 66 exercise.

67 Keywords: blood flow; cooling; muscle damage; inflammation

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73 INTRODUCTION

74 Lower limb cold-water immersion (CWI) is a widely used recovery method 75 to reduce the negative symptoms associated with high-intensity or unaccustomed 76 exercise (Bailey et al., 2007; Leeder, Gissane, van Someren, Gregson & Howatson, 2012). Cooling of the exercised muscles is proposed to attenuate acute inflammation, 77 78 edema and swelling, thereby reducing the development of exercise-induced muscle 79 damage, function and soreness (Smith, 1991). Previous studies have shown that CWI 80 decreases limb muscle temperature and blood flow when applied at rest (Gregson et 81 al., 2011) and following continuous endurance exercise such as cycling (Mawhinney 82 et al., 2013; Vaile et al., 2011) and treadmill running (Ihsan, Watson, Lipski & 83 Abbiss, 2013). The effect of CWI on the physiological and functional responses to 84 resistance type exercise are less well known.

85 Recent research has shown that the chronic application of CWI (2 $d \cdot w^{-1}$ over 86 12 weeks) after resistance exercise reduces resistance training-induced increases in 87 muscle strength and mass compared with an active cool-down due to the blunting of 88 cellular signaling (Roberts et al., 2015b). On the contrary, in the acute period, i.e. 89 hours, after CWI application, increases in muscle function relative to active recovery 90 have been reported (Roberts et al., 2015a). The improved recovery of strength with 91 acute CWI was modulated by muscle temperature and potentially blood flow (muscle 92 oxygenation) (Roberts et al., 2015a). Nevertheless, no study, to date has directly 93 examined the impact of CWI on limb blood flow following an acute bout of resistance 94 exercise. This is important to establish, since resistance exercise can cause a different 95 haemodynamic, thermoregulatory and mechanical stress than endurance exercise. For 96 example, the metabolic cost of muscle contraction is prolonged during activities such 97 as running and cycling, rather than intermittent during resistance exercise, with

98 skeletal muscle blood flow matched to the metabolic demands of the contracting 99 muscle (Joyner & Casey, 2015). Similarly, the intermittent nature and potential for 100 breath holding in resistance exercise contrasts the linear increase and plateau in limb 101 blood flow in endurance exercise (MacDougall et al., 1992; Mortensen, Damsgaard, 102 Dawson, Secher & Gonzalez-Alonso, 2008). It is also possible that resistance exercise 103 does not cause increases in core body temperature of the same magnitude as 104 endurance exercise (Deschenes et al., 1998). A higher core body temperature may 105 increase tissue-cooling rate due to a greater temperature gradient between the body 106 and the water (Stephens, Halson, Miller, Slater & Askew, 2016). Moreover, 107 resistance exercise stimulates greater muscle damage compared with other modes of 108 exercise, such as cycling and running (Dolezal, Potteiger, Jacobsen & Benedict, 2000; 109 Howatson et al., 2012).

110 We have previously shown that CWI of various water temperatures similarly 111 decreases post-cycling lower limb blood flow despite greater reductions in muscle 112 and thigh skin temperatures in colder water (Mawhinney et al., 2013). It is currently 113 unknown if the differences in hemodynamic and temperature responses mediated by 114 resistance, relative to endurance, exercise, would impact upon post-resistance 115 exercise responses to CWI and if different water temperatures of CWI would result 116 in similar or graded decreases in limb blood flow after resistance exercise. Therefore, 117 the aim of this study was to examine the effects of cold (8°C) and cool (22°C) water 118 immersion on lower limb blood flow and muscle temperature changes, after a typical 119 bout of resistance exercise.

121 MATERIALS AND METHODS

122 **Participants**

123 Twelve recreationally active men who were non-smokers and free from 124 cardiovascular, respiratory and metabolic disease were studied (mean $\pm s$: age, 26 ± 6 125 yrs; height, 1.8±0.1 m; mass, 77.5±11.2 kg; 10-repetition maximum (10 RM), 126 50.4±13.4 kg). The participants typically performed resistance exercise at least three 127 times per week and performed squat exercise at least once per week in their training 128 regime (self-report questionnaire). The participants were familiarized with the 129 experimental procedure and associated risks and gave their written informed consent 130 to participate. The study was approved by the Institutional Ethics Committee and 131 conformed to the 1964 Declaration of Helsinki and its later amendments for research 132 using human participants.

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134 Experimental Design

135 Two weeks prior to the commencement of the experimental trials, each participant 136 completed a 10 RM parallel depth squat assessment using a Smith machine 137 (Familiarization 1). The squat protocol consisted of a warm up set, using only the bar, 138 followed by progressive increases in load until the attainment of the 10 RM within 139 five attempts (Baechle & Earle, 2000). The following week, participants completed 140 4 sets of the predetermined 10 RM squat exercise interspersed with 2 min rest periods 141 (Familiarization 2). This second familiarization trial was performed to reduce the 142 magnitude of any subsequent muscle damage and inflammation from the exercise 143 stimulus in the proceeding trials, e.g., reduce an order effect, that might influence 144 blood flow, which is commonly known as the protective repeated bout effect 145 (Howatson & van Someren, 2008).

146 The experimental trials were performed in a randomized counterbalanced 147 order, at least 7-days following the second familiarization session and at least 7-days 148 apart. For each trial, participants arrived at the laboratory at least 3 h postprandial, 149 having refrained from exercise, alcohol, tobacco and caffeine during the previous 24 h and having consumed 5 ml·kg⁻¹ of water 2 h before arrival. All participants recorded 150 151 their nutritional and fluid intake for 24 h prior to their first experimental trial. This 152 record was photocopied and returned to them to repeat for their remaining trials. All 153 trials were conducted under an ambient temperature of 22-24°C to control variability 154 in cutaneous blood flow (Cracowski, Minson, Salvat-Melis & Halliwill, 2006) and at 155 the same time of day in order to avoid the circadian variation in internal body 156 temperature.

157 Each participant was required to complete 4 sets of 10 RM squats followed 158 by a 10 min period of immersion in either 8°C or 22°C water or seated rest (Control). 159 The water temperatures and immersion protocol was based on our previous studies 160 (Gregson et al., 2011; Mawhinney et al., 2013). On arrival, nude body mass (kg) was 161 obtained (Seca, Hamburg, Germany). A rectal probe was self-inserted and a heart rate 162 (HR) monitor was positioned across the chest. Participants then rested supine for 30 163 min for instrumentation and to stabilize physiological status, wearing training shorts. 164 Following baseline measurements (10 min), participants completed 4 sets of 10 RM 165 squats interspersed with a 2 min rest period between sets. Participants then returned 166 to the supine position for 10 min for post-exercise/pre-immersion measurements. 167 Participants were then raised from the bed in a semi-recline position using an 168 electronic hoist (Bianca, Arjo Ltd, Gloucester, United Kingdom) and either lowered 169 into the water tank (ECB, Gloucester, U.K.) to the iliac crest for 10 min, or remained 170 suspended above the bed (Control). At the end of immersion, participants were

returned to the bed using the electronic hoist and remained supine for 30 min. The
use of the hoist to raise and lower the participants was important to avoid the effect
of muscle activation on blood flow

174 Rectal and skin temperatures, HR and thigh and calf cutaneous blood flow 175 were continuously monitored. Muscle temperature, superficial femoral artery blood 176 flow and mean arterial blood pressure (MAP) were measured at baseline, preimmersion and during post immersion. At the same time points, both perceived 177 178 thermal comfort, rated using a 9-point scale (0 = unbearably cold to 9 = very hot)179 (Young, Sawka, Epstein, Decristofano & Pandolf, 1987) and shivering, rated using a 180 4-point scale (1 = no shivering to 4 = heavy shivering) (Wakabayashi, Hanai, 181 Yokoyama & Nomura, 2006) were recorded.

182

183 Measurements

184 *Rectal, Thigh, Skin, and Muscle Temperatures*

185 A rectal probe (Rectal probe (adult), Ellab UK, Norwich, England) was 186 inserted 15 cm beyond the anal sphincter for the assessment of rectal temperature. 187 Skin thermistors (Surface temperature probe (stationary), Ellab UK, Norwich, 188 England) were attached to the chest, forearm, upper thigh, and calf for the assessment 189 of local and mean skin temperature (Ramanathan, 1964). Muscle temperature was 190 assessed using a needle thermistor inserted into the vastus lateralis (Multi-purpose 191 needle probe, Ellab UK, Norwich, England). Thigh skinfold thickness was measured 192 using Harpenden skinfold calipers (HSK BI, Baty International, West Sussex, United 193 Kingdom) and divided by 2 to determine the thickness of the thigh subcutaneous fat 194 layer over the vastus lateralis (Enwemeka, et al., 2002). The needle thermistor was 195 inserted at a depth of 3 cm plus one-half the skinfold measurement for determination of deep muscle temperature (3 cm). The thermistor was then withdrawn at 1 cm increments for determination of muscle temperature at 2 cm and 1 cm below the subcutaneous layer. Rectal, skin and muscle temperatures were recorded using an electronic measuring system (E-Val Flex, TMN9616, Ellab UK, Norwich, England).

201 Heart Rate and Arterial Blood Pressure

HR was continuously measured using short-range telemetry (S610; Polar
Electro Oy, Kempele, Finland). Arterial blood pressure was measured via automated
brachial auscultation (Dinamap, GE Pro 300V2, Tampa, Florida, USA), and MAP
was calculated as [Diastolic + (0.333 x (Systolic-Diastolic))].

206

207 Femoral Artery Blood Flow

208 A 15 MHz multi-frequency linear array transducer attached to a high-209 resolution ultrasound machine (Acuson P50, Siemens, Germany) was used to 210 measure femoral artery diameter and velocity. Images were taken at the superficial 211 femoral artery in the proximal third of the left leg approximately 3 cm distal to the 212 bifurcation. This position was marked on the skin for ultrasound head repositioning 213 during repeated measures. Ultrasound parameters were set to optimize longitudinal 214 B-mode images of the lumen/arterial wall interface. Continuous and synchronized 215 pulsed wave Doppler velocities were also obtained. Data were collected using an 216 insonation angle of 60° and each measurement was recorded for 2 min. Analysis of 217 blood flow velocity and diameter was performed using custom designed edge-218 detection and wall-tracking software (Green, Cheetham, Reed, Dembo & O'Driscoll, 219 2002; Thijssen et al., 2011; Woodman et al., 2001). Blood flow was calculated as the 220 product of cross-sectional area and blood flow velocity. Resting diameter, blood flow

velocity and blood flow were sampled as the mean of a 20 s period of each 2 minimage. Femoral vascular conductance was calculated as the ratio of blood flow/MAP.

223

224 Cutaneous Blood Flow

225 Red blood cell flux was used as an index of skin blood flow via laser Doppler 226 flowmetry (Periflux System 5001, Perimed Instruments, Jarfalla, Sweden). An 227 integrated laser Doppler probe (Probe 413, Perimed, Suffolk, United Kingdom) was 228 attached to the mid-anterior thigh halfway between the inguinal line and the patella, 229 and on the calf in the region of the largest circumference. Once affixed, the probes 230 were not removed until the completion of each trial. Cutaneous vascular conductance 231 was calculated as the ratio of laser Doppler flux to MAP (cutaneous vascular 232 conductance = laser Doppler flux/MAP x 100) and expressed as a percentage change 233 from pre immersion values. Thigh and calf skin conductance are expressed as 234 percentage change from pre immersion (zero)

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236 Statistical Analysis

237 It was estimated that a sample size of at least 6 participants would have 90% power to detect a 175 ml·min⁻¹ reduction in femoral artery blood flow following 10 238 239 min of cool (22°C) water immersion, using a standard deviation of the differences of 240 99 ml·min⁻¹ (Mawhinney et al., 2013). A two-factor (condition x time) general linear 241 model (GLM) was used to evaluate treatment differences between the 8°C, 22°C and 242 control conditions. A three-way GLM (condition x depth x time) was employed to 243 analyse muscle temperature. Significant main effects and interactions were followed 244 up using multiple comparisons (Student-Newman-Keuls). The α level for evaluation of statistical significance was set at P < 0.05 and were analysed using Statistical Package for the Social Sciences (Chicago, IL). All data are presented as mean±s.

247

248 **RESULTS**

249 *Thermoregulatory responses*

Exercise elicited an increase in rectal temperature (8°C; $\Delta 0.3\pm0.2$ °C; 22°C; $\Delta 0.2\pm0.1$ °C; control; 0.3 ± 0.1 °C; *P* < 0.001) but rectal temperature was not different between conditions (*P* > 0.05; Figure 1a). Rectal temperature decreased over the post immersion recovery period (*P* < 0.001) with no difference observed between conditions (*P* = 0.19; Figure. 1a).

255 Exercise elicited an increase in thigh (8°C; $\Delta 0.4\pm0.6$ °C; 22°C; $\Delta 0.8\pm0.6$ °C; 256 control; $\Delta 0.6\pm 0.8^{\circ}$ C; P = 0.002) and mean skin temperature (8°C; $\Delta 0.3\pm 0.2^{\circ}$ C; 257 22°C; $\Delta 0.2\pm0.1$ °C; control; 0.3 ± 0.1 °C; P < 0.001) but skin temperatures were not 258 different between conditions (P > 0.05; Figure. 1). The colder water reduced local 259 thigh and mean skin temperatures to a greater extent compared to 22°C throughout 260 post-immersion (P < 0.001; Figure 1); both skin temperatures were lower in both 261 cooling conditions compared with the control condition. Both temperatures gradually 262 increased during the 30 min recovery period in both cooling conditions whilst values 263 remained relatively stable in the control condition. Local thigh and mean skin 264 temperature remained below baseline at the end of the recovery period in the 8°C and 265 22°C conditions (P < 0.001) and were unchanged in the control condition (P > 0.05; 266 Figure. 1).

Exercise induced increases in muscle temperature at 3 cm (8°C; $\Delta 0.8\pm0.3$ °C; 268 22°C; $\Delta 1.4\pm0.5$ °C; control; $\Delta 1.0\pm0.4$ °C), 2 cm (8°C; $\Delta 0.9\pm0.4$ °C; 22°C; $\Delta 1.3\pm0.7$ °C; control; $\Delta 1.1\pm0.6$ °C), and 1 cm (8°C; $\Delta 1.0\pm0.6$ °C; 22°C; $\Delta 1.2\pm0.9$ °C;

control; $\Delta 1.1\pm0.7^{\circ}$ C) depths (*P* < 0.001), which were similar between conditions (*P* > 0.05; Figure. 2). During the post immersion recovery period, a greater reduction in muscle temperature was observed in both cooling conditions compared with the control condition at all 3 probe depths and at each time point (*P* < 0.001; Figure 2). There was also a greater reduction in muscle temperature at each depth in 8°C cooling compared with 22°C at each time point (*P* < 0.001; Figure 2).

276 Thermal comfort was lower after cooling; both immediately ($8^{\circ}C$, 2 ± 1 AU; 277 22°C, 3 ± 1 AU; control, 5 ± 1 AU, P < 0.001) and 10 min post immersion (8°C, 3 ± 1 AU; 22° C, 4 ± 1 AU; control, 5 ± 1 AU, P < 0.01) compared with the control condition. 278 279 A lower thermal comfort rating also occurred in the 8°C condition, 20 min after 280 immersion, compared with the control condition (P < 0.001). Thermal comfort was 281 also lower in the colder water compared with 22°C for up to 10 min after immersion 282 (P < 0.001). There was no difference in thermal comfort between conditions at the 283 end of the 30 min recovery period (P > 0.05) with similar ratings to baseline. Slight 284 to moderate shivering was observed during immersion in both cooling conditions 285 compared with no shivering in control (8°C, 2±1 AU; 22°C, 2±1 AU; control, 1±0 286 AU). There was no shivering observed throughout the post immersion period in any 287 experimental condition.

288

289 *Heart rate, mean arterial pressure and ratings of perceived exertion (RPE)*

Each set of 10 repetitions of squat exercise increased HR (P < 0.01), which remained elevated prior to immersion (8°C; 77±11 beats·min⁻¹; 22°C; 73±11 beats·min⁻¹; control; 73±10 beats·min⁻¹; P < 0.001). HR was increased during colder water immersion (8°C, 80±14 beats·min⁻¹; 22°C, 69±9 beats·min⁻¹; control; 71±7

beats·min⁻¹; P < 0.001), but remained similar between all conditions during the post immersion recovery period (P > 0.05).

296 MAP was not different between conditions immediately prior to immersion 297 (8°C; 89±5 mmHg; 22°C; 88±5 mmHg; control; 88±6 mmHg; *P* > 0.05). MAP was 298 higher during the 10 min immersion period and immediately post immersion in 8°C 299 water (95±7 mmHg) compared to 22°C, (88±7 mmHg) and control (87±4 mmHg) 300 conditions (P < 0.01). MAP was similar between all conditions throughout the 301 remaining period of the post immersion phase (P > 0.05). MAP returned towards 302 baseline values at the end of the 30 min recovery period in the 22°C and control 303 conditions (P > 0.05), but still remained elevated in the 8°C condition (8°C, 90±6; 304 22°C, 90±5; control, 89±7 mm Hg; *P* = 0.02).

305 RPE was similar between trials in the first set of exercise (8°C; 13±2 AU; 306 22°C; 13±1 AU; control; 13±1 AU; P > 0.05). There was a higher rating with each 307 subsequent set of squat exercise (P < 0.001) with RPE remaining similar between 308 conditions until the end of exercise (8°C; 15±2 AU; 22°C; 15±2 AU; control; 15±2 309 AU; P > 0.05).

310

311 *Femoral artery and cutaneous blood flow responses.*

Exercise increased femoral blood flow and conductance by ~75% and ~80% respectively (P < 0.001) which was not different between conditions (P > 0.05; Figure 3). A lower femoral artery blood flow and conductance (~50%) was observed during post-immersion recovery period in both cooling conditions compared with control (8°C, 22°C, P < 0.01; Figure 3). Cooling reduced femoral artery blood flow and conductance by ~60% and ~75% relative to baseline and pre-immersion values, respectively, at the end of the 30 min recovery period. Pre-immersion thigh (8°C, 0.23±0.15 AU; 22°C, 0.28±0.21 AU; control, 0.31±0.15 AU; P = 0.31) and calf (8°C, 0.22±0.20 AU; 22°C, 0.16±0.10 AU; control, 0.17±0.08 AU; P = 0.45) cutaneous vascular conductance were not different between conditions. A greater skin vasoconstriction was observed in both cooling conditions at the thigh (P < 0.01) and calf (P < 0.01) relative to the control throughout the postimmersion recovery period (~50-60%; P > 0.05). No differences were observed between cooling conditions (Figure 4).

326

327 **DISCUSSION**

328 The purpose of this study was to investigate the effects of CWI of various 329 water temperatures on lower limb blood flow following resistance exercise. We found 330 no differences in the blood flow responses to CWI at 8°C and 22°C following 331 resistance exercise despite greater reductions in muscle and skin temperatures after 332 CWI of 8°C. Moreover, these responses were similar in time course and magnitude 333 to our previous findings following endurance cycling exercise (Mawhinney et al., 2013). Taken together, these findings suggest that the application of CWI is similarly 334 335 effective with regards to vascular responses following different modes of moderate 336 intensity exercise.

Previous studies, which have examined the influence of CWI on limb blood flow responses after exercise, have used an endurance exercise stimulus (Ihsan et al., 2013; Mawhinney et al., 2013; Vaile et al., 2011). These endurance type protocols typically produce a greater level of systemic (e.g., core temperature) hyperthermia and different metabolic perturbations, compared with resistance exercise (Deschenes et al., 1998; Mortensen et al., 2008). A relative decrease in blood volume in the leg muscle microcirculation after CWI of 10°C has been reported after knee extensor

344 resistance exercise using near-infrared spectroscopy (Roberts et al., 2015a), however, 345 this method is associated with several limitations (Davis, Fadel, Cui, Thomas & 346 Crandall, 2006; Ferrari, Mottola & Quaresima, 2004) compared with absolute 347 measures of femoral and skin blood flow. In the present study, 10-min of lower body 348 immersion in either 8°C or 22°C water reduced femoral artery blood flow by ~75% 349 and ~50%, respectively, compared with the control condition. The magnitude of 350 change in femoral artery conductance after CWI was similar to our previous 351 observations (~55%) after cycling exercise (Mawhinney et al., 2013) and other 352 studies, which assessed limb blood flow with other methods (Ihsan et al., 2013; Vaile 353 et al., 2011). The lack of difference in the femoral artery conductance response to 354 cold (8°C) and cool (22°C) water in the current study, despite greater decreases in 355 muscle temperature in cold water, are in agreement with our previous work (Gregson 356 et al., 2011; Mawhinney et al., 2013) and are likely due to an insufficiently large 357 enough difference in deep muscle temperature between cooling conditions ($\sim 1^{\circ}C$) to 358 directly modify femoral artery blood flow.

359

360 It has previously been observed that heat stress from cycling exercise 361 (Mawhinney et al, 2013) can cause a different cutaneous blood flow response to CWI 362 compared with resting conditions (Gregson et al, 2011), e.g., a lack of difference in 363 cutaneous vasoconstriction after immersion in cold and cool water temperatures 364 following cycling exercise. However, it remains to be elucidated whether a smaller 365 level of thermal strain after a bout of resistance exercise could influence the cutaneous 366 blood flow response to CWI. This is important to establish because a greater 367 cutaneous blood flow during cooling may infer less muscle blood flow (Gregson et 368 al, 2011). In the present study, rises in core ($\sim 0.3^{\circ}$ C) and local limb temperatures

369 (muscle 3 cm, ~1°C; skin, ~0.6°C) after resistance exercise led to increases in thigh 370 and calf cutaneous vascular conductance. Despite differences in lower limb skin temperature after immersion in 8°C and 22°C water, reductions in lower limb 371 372 cutaneous vascular conductance were similar between cooling conditions and in 373 agreement with our previous work (Mawhinney et al, 2013) that elicited a higher 374 thermoregulatory strain (core 0.9°C, muscle 3 cm; 1.6°C and skin 1.7°C). It is 375 therefore conceivable that only a small hyperthermic load (systemic or local limb) is 376 required to blunt cutaneous vasoconstrictor responsiveness (Wilson, Cui & Crandall, 377 2002). In addition, cold-induced vasodilation can occur in 8°C water, albeit under 378 resting conditions with no change in body temperature, which may contribute to a 379 similar skin blood flow after 8°C CWI relative to 22°C CWI (Gregson et al, 2011). In 380 combination, similar changes in femoral artery and cutaneous blood flow after CWI 381 in 8°C and 22°C water suggest that both cooling conditions will be equally effective 382 in reducing blood flow when applied after resistance exercise and that the 22°C water 383 may be more tolerable based on the increased thermal comfort ratings in this 384 condition.

385

386 It is difficult to directly measure muscle blood flow in humans, particularly 387 across a broad area of muscle. Our approach, measuring total limb and cutaneous 388 blood flow simultaneously, allows some inferences to be drawn regarding generalized 389 changes in blood flow to muscle. In response to cooling in the present experiment, 390 changes in both total limb and cutaneous flow were similar. This suggests that despite 391 distinct impacts of 8°C and 22°C cooling on skin and muscle temperatures (especially 392 deeper muscle temperatures), the impact on muscle blood flow was qualitatively 393 similar. Collectively, these data infer that, if different degrees of post-exercise cooling have an impact upon recovery following resistance training, they are independent ofblood flow to muscle.

396

397 Muscle temperature-induced reductions in microvascular blood flow may 398 reduce inflammation, edema, swelling and pain after tissue injury and limit secondary 399 injury (Lee et al, 2005). The proposal that cooling induced reductions in limb blood 400 flow are beneficial in limiting the inflammatory response after muscle damaging 401 exercise is largely based on animal research, which has shown muscle cooling to 402 reduce markers of inflammation in damaged muscle (Lee et al, 2005; Ramos et al, 403 2016; Schaser et al, 2007). A recent novel study using humans has recently challenged 404 this view by showing that CWI (10 min at 10°C), applied after lower body resistance 405 exercise, has no impact on the muscle inflammatory or cellular stress response 406 compared with active recovery (Peake et al, 2016). Additionally, the chronic application of CWI (2 d·w⁻¹ over 12 weeks) applied after resistance-training exercise 407 408 also blunts the cellular adaptation responses and long-term gains in muscle mass and 409 strength (Roberts et al, 2015b). Nevertheless, a reduction in muscle blood flow may 410 still provide benefits to the acute recovery of muscle function after resistance exercise 411 (Roberts et al., 2015a) by attenuating edema and swelling per se (Dolan, Thornton, 412 Fish & Mendel, 1997; Yanagisawa, et al, 2003) and associated pain (e.g. soreness) 413 upon movement (Diong & Kamper, 2014). These findings have implications for the 414 use of CWI in the periodization of training. For example, CWI may be better utilized 415 in situations where repeated bouts of intense resistance exercise are required in short periods of time rather than as a regular adjunct to resistance training. 416

417

418 In line with our previous observations (Gregson et al, 2011; Mawhinney et al,

2013), the increases in MAP and HR during 8°C immersion are characteristic of the 419 420 well-established cold pressor response (Victor, Leimbach, Seals & Wallin, 1987). 421 The changes in these cardiovascular indices are initiated by the activation of noxious 422 skin thermonociceptors that cause a reflex increase in sympathetic nervous activity 423 leading to peripheral vasoconstriction and reductions in arterial blood flow (Gregson 424 et al, 2011). In the 22°C condition, there was no observed increase in HR or MAP 425 despite a reduction in limb blood flow. These findings are consistent with the 426 activation of non-noxious thermonociceptors operable at similar temperatures 427 (Gregson et al, 2011). The stimulation of these particular thermonociceptors are 428 related to the difference in skin temperatures and ratings of thermal sensation during 429 immersion in the different cooling conditions.

430

431 In the present study, seated rest in ambient air was selected as the control; 432 consequently, the effect of hydrostatic pressure on limb blood flow per se, 433 independent of the water temperature effect, was not assessed. The pressure effect of 434 water has previously been shown to increase femoral artery blood flow by ~250-300 435 ml·min⁻¹ in thermoneutral immersion under non-exercise conditions (Ménétrier et al, 436 2015). Therefore, in our study, it is possible that the hydrostatic effect of water per 437 se may have prevented a greater magnitude of decrease in arterial blood flow being 438 observed after cooling.

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440

441 CONCLUSION

The application of lower limb immersion in 8°C and 22°C water after a bout
of resistance exercise decreases femoral artery and cutaneous blood flows compared

with rest and to a similar extent between cold and cool water temperatures.
Individuals who may not tolerate colder water temperatures may therefore use less
noxious water temperatures after resistance exercise. These findings have practical
implications for the acute use of cold-water immersion for recovery in clinical and
athletic settings.

449

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453

454 **DISCLOSURE STATEMENT**

455 WG has received funding from ECB Cold Spas Ltd for the CWI facility and from UK

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457 of interest.

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635 Figure 1. Rectal temperature (A), mean skin temperature (B) and thigh skin temperature (C) pre and post immersion in 8°C, 22°C and control (n = 12, mean \pm 636 SD). Main effects for condition (P < 0.001) and time (P < 0.001), alongside a 637 638 significant interaction between condition and time (P < 0.001), were found for thigh 639 and mean skin temperature. Main effects for time (P < 0.001) were found for rectal 640 temperature. Significant difference from baseline in the 8°C condition (*), 22°C condition (**) and control conditions (***) (P < 0.01). Significant difference between 641 cooling conditions vs control (+) (P < 0.001). Significant difference between cooling 642 conditions (#) (*P*<0.05). 643

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Figure 2. Muscle temperature pre and post immersion, at temperature probe depths of 3 cm (A), 2 cm (B), and 1cm (C) (n =12, mean \pm SD). Main effects for condition (*P*<0.001) and time (*P*<0.001) were found along with a significant interaction between condition, time and probe depth (*P*<0.001). Significant difference from baseline in the 8°C (*), 22°C (**) and control conditions (***) (*P*<0.001). Significant difference between cooling conditions vs control (+) (*P*<0.001). Significant difference between cooling conditions (#) (*P*<0.05).

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Figure 3. Femoral artery blood flow (A) and conductance (B) pre and post immersion in 8°C, 22°C and control (n = 12, mean \pm SD). A main effect for condition (*P*<0.001) and time (*P*<0.001) was found for both artery flow and conductance. There was also a significant interaction between condition and time for both artery flow (*P*<0.01) and conductance (*P*<0.01). Significant difference from baseline in the 8°C (*), 22°C (**) and control conditions (***) (*P*<0.05). Significant difference between cooling conditions vs control (+) (*P*<0.01).

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661 Figure 4. Percentage change in thigh cutaneous vascular conductance (A) and calf 662 vascular conductance (B) from pre immersion in 8° C, 22° C and control (n = 12, mean 663 \pm SD). Main effects for condition (P<0.01) were found for both thigh and calf cutaneous vascular conductance. A main effect for time (P < 0.05) was also found for 664 thigh conductance. There were no interactions between condition and time in thigh 665 666 (P=0.78) or calf vascular conductance (P=0.42). Significant difference from baseline in the 8°C (*), 22°C (**) and control conditions (***) (P<0.05). Significant 667 668 difference between cooling conditions vs control (+) (P < 0.01).