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1 **A new proof-of-concept in bacterial reduction: Antimicrobial action of**  
2 **violet-blue light (405 nm) in ex vivo stored plasma**

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13 **Running Heading:** Decontamination of blood plasma using 405nm light

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22 **ABSTRACT**

23 Bacterial contamination of injectable stored biological fluids such as blood plasma and  
24 platelet concentrates preserved in plasma at room temperature is a major health-risk. Current  
25 pathogen-reduction technologies (PRT) rely on the use of chemicals and/or ultraviolet-light,  
26 which affects product quality and can be associated with adverse events in recipients. 405nm  
27 violet-blue light is antibacterial without the use of photosensitizers, and can be applied at  
28 levels safe for human exposure, making it of potential interest for decontamination of  
29 biological fluids such as plasma.

30 As a pilot study to test whether 405nm light is capable of inactivating bacteria in biological  
31 fluids, rabbit and human plasma were seeded with bacteria and treated with a 405nm light  
32 emitting diode (LED) exposure system (patent pending). Inactivation was achieved in all  
33 tested samples, ranging from low volumes to pre-bagged plasma. 99.9% reduction of low  
34 density bacterial populations ( $\leq 10^3$  CFUml<sup>-1</sup>), selected to represent typical ‘natural’  
35 contamination levels, were achieved using doses of 144 Jcm<sup>-2</sup>.

36 The penetrability of 405nm light, permitting decontamination of pre-bagged plasma, and the  
37 non-requirement for photosensitizing agents, provides a new proof-of-concept in bacterial  
38 reduction in biological fluids, especially injectable fluids relevant to transfusion medicine.

39 **(Word count: 190)**

40

41 **KEY WORDS:** Plasma; Decontamination; 405nm light; violet-blue light; transfusion bags;  
42 pathogen reduction technology; Bacteria; Contamination

43

## 44 INTRODUCTION

45 Bacterial contamination of ex vivo stored injectable biological fluids such as blood and blood  
46 components preserved in plasma is a major complication for transfusion medicine, resulting  
47 in both wasteful discarding of valuable blood products, and more significantly, health risks  
48 for recipients of contaminated donor blood [1,2]. Major progress has been made in the  
49 provision of a safe supply of blood components, and measures such as more effective donor  
50 screening, extensive laboratory testing protocols and the application of bacterial reduction  
51 methods have significantly reduced the risk of transfusion-transmitted bacterial infections [1-  
52 3]. Nevertheless, the risk of bacterial transmission has not been completely eliminated and  
53 there is a recognised need for continued research to improve the efficacy of these methods,  
54 and to minimise incidental adverse changes in biological fluids, such as cellular blood  
55 components preserved in plasma, that can compromise product quality and safety [4-6].

56 A number of bacterial reduction methods have been developed for plasma treatment, and  
57 pathogen-reduced plasma is routinely used [7], with several of these methods now licensed  
58 for use in North America and Europe [5]. The original methods developed for plasma  
59 treatment included the use of solvent/detergent, and methylene blue in combination with  
60 visible light [8-11]. More recently developed methods have employed ultraviolet (UV) light.  
61 Exposure to amotosalen (S-59) plus long-wave ultraviolet (UVA) light [12,13], and treatment  
62 with riboflavin and UV light [7,14], have been developed to treat both plasma and platelets.  
63 Whilst light-based processes have typically used photosensitive chemicals to generate  
64 microbicidal effects, a UVC-based pathogen reduction system without a requirement for  
65 photoactive substances has been developed and is undergoing clinical efficacy and safety  
66 testing [15-17].

67 It is generally accepted that all these methods have limitations [5,7], and because the full  
68 extent of future microbiological challenges cannot be predicted, pathogen reduction  
69 technologies will remain an active area of investigation in transfusion medicine well into the  
70 future [1,4].

71 Here we report the first proof-of-concept results on the use of a novel visible violet-blue light  
72 method that does not require the addition of photosensitive chemicals for inactivation of  
73 bacterial pathogens in plasma. This method utilises light with a peak wavelength of 405 nm,  
74 which causes photoexcitation of endogenous microbial porphyrin molecules and oxidative  
75 damage through reactive oxygen species [18]. 405 nm light has previously been shown to  
76 inactivate a wide range of bacterial pathogens in laboratory tests [19-28], as well as in  
77 hospital settings with use as an environmental disinfection technology [29-31], and also  
78 potential for wound decontamination applications in clinical settings [33-35]. An advantage  
79 of this technology over UV-light for certain applications is that, even at irradiance values and  
80 dose levels that are bactericidal, it can be applied safely for human exposure. Therefore, we  
81 envisioned that this feature makes 405 nm light of potential interest for decontamination of  
82 injectable stored biological fluids such as blood plasma or plasma containing cellular blood  
83 components. Tests on bacterial-seeded plasma were carried out on both small-scale liquid  
84 samples and artificially-contaminated pre-bagged plasma. Direct treatment of pre-bagged  
85 plasma was facilitated by the highly transmissible properties of 405 nm light, and the  
86 bacterial inactivation results obtained using this novel approach are described for the first  
87 time in this paper.

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89

90

## 91 MATERIALS AND METHODS

92 **Bacterial Cultures:** The organisms used in this study were *Staphylococcus aureus* NCTC  
93 4135, *Staphylococcus epidermidis* NCTC 11964 and *Escherichia coli* NCTC 9001. Cultures  
94 were obtained from the National Collection of Type Cultures (NCTC), Collindale, UK. For  
95 experimental use, bacteria were cultured in 100 ml nutrient broth at 37°C under rotary  
96 conditions (120 rpm) for 18-h. Broths were centrifuged at  $3939 \times g$  for 10 minutes and the  
97 pellet re-suspended in 100 ml phosphate buffered saline (PBS), and serially diluted to obtain  
98 the required cell density (colony-forming units per millilitre, CFU ml<sup>-1</sup>) for experimental use.  
99 All culture media was sourced from Oxoid Ltd (UK).

100 **Plasma:** Lyophilised rabbit plasma (LRP020, E&O Laboratories, UK) was reconstituted  
101 using sterile distilled water. Fresh frozen human plasma (approximately 300 ml bag volume)  
102 was obtained from the Scottish National Blood Transfusion Service (SNBTS, UK), and  
103 defrosted before experimental use. Study involving human subjects protocol was approved  
104 by FDA Risk Involved in Human Subjects Committee (RIHSC, Exemption Approval # 11-  
105 036B) and by the University of Strathclyde Ethics Committee (letter dated February 10,  
106 2011). Rabbit and human plasma suspensions were seeded with known concentrations of  
107 bacterial contaminants by adding bacterial-PBS suspension to the plasma.

108 **405-nm light source:** The 405 nm light sources used were rectangular arrays of 99-LEDs in  
109 an 11 × 9 matrix (Optodiode Corp, USA). The array had a centre wavelength close to  
110 405 nm, with a bandwidth of approximately 10 nm at full-width half maximum (FWHM).  
111 The LED array was powered by a direct current supply, and for thermal management, the  
112 LED array was bonded to a heat sink and fan, thus ensuring that heating had no effect on the  
113 test samples exposed to the 405-nm light (Device patent pending [36]).

114 **405 nm antimicrobial light treatment:** Three arrangements were employed for  
115 exposure of three different sample volumes: 3 ml, 30 ml and approximately 300 ml (whole  
116 plasma transfusion bags). For exposure of 3 ml sample volumes, the samples were held in  
117 the well of a 12-well microplate (without the lid), and the LED array was mounted in a  
118 polyvinyl chloride (PVC) housing which positioned the array approx. 3 cm directly above the  
119 sample. Irradiance at the sample surface was measured to be approximately  $100 \text{ mWcm}^{-2}$   
120 (measured by using a radiant power meter and photodiode detector; L.O.T.-Oriol Ltd.).

121 For exposure of 30 ml sample volumes, the human plasma was held in a sterile 90 mm Petri  
122 dish with the lid on. The LED array was positioned 8 cm directly above the closed sample  
123 dish, providing an irradiance of approximately  $8 \text{ mWcm}^{-2}$ , through the lid, at the centre of the  
124 sample dish.

125 For exposure of plasma bags, a test rig was constructed which held two 405 nm LED arrays  
126 at a distance of 12 cm above the horizontally-positioned plasma bag. This arrangement  
127 provided an irradiance of approximately  $5 \text{ mWcm}^{-2}$  at the centre position of the plasma bag,  
128 taking into account a 20% reduction in irradiance as the light transmits through the bag layer.

129 In order to investigate the influence of higher irradiances on bacterial inactivation, plasma  
130 bags were also exposed using irradiances of 16 and  $48 \text{ mWcm}^{-2}$ . These higher irradiances  
131 were achieved by using two high-power 405 nm LED arrays (PhotonStar Technologies, UK),  
132 with 14 nm FWHM.

133 All experimental systems were held in a shaking incubator (72 rpm;  $25^{\circ}\text{C}$ ) to allow  
134 continuous sample agitation and maintain exposure conditions. Samples seeded with  
135 bacterial contamination were treated with increasing exposures of 405 nm light. Control  
136 samples were held in identical conditions, but shielded from the 405 nm light.

137 The optical profiles of the light distribution across the Petri dishes and transfusion bags  
138 (plotted using MATLAB R2012b software) demonstrate the non-uniform irradiance of the  
139 plasma (Figs 2a, 3a), however, continuous agitation of the plasma samples during treatment  
140 ensure uniform mixing of the plasma contaminants. Negligible variation was recorded across  
141 the 22 mm  $\varnothing$  of the 3 ml samples.

142 **Determination if Light Induces Toxicity within Human Plasma:** To ensure that bacterial  
143 inactivation was not the result of the plasma becoming toxic upon exposure to 405 nm light,  
144 *S. aureus* ( $1 \times 10^3$  CFUml<sup>-1</sup>) was seeded into 3 ml plasma that had been pre-exposed to  
145  $1.08 \text{ kJcm}^{-2}$  405 nm light at an irradiance of  $100 \text{ mWcm}^{-2}$  (the highest dose employed in the  
146 present study) and samples were taken at 30-min intervals for up to 3-hr.

147 **Bacterial Enumeration:** Following 405 nm light exposure, samples were plated onto  
148 nutrient agar using either an automatic spiral plater (Don Whitley Scientific, UK) or manually  
149 spread by using sterile L-shaped spreaders, depending on the expected population density of  
150 the samples. Sample plates were incubated at 37°C for 24 hours, and then enumerated with  
151 the surviving bacterial load reported as colony-forming units per millilitre (CFUml<sup>-1</sup>).

152 **Inactivation Data Analysis:** Results are reported as surviving bacterial load ( $\log_{10}$  CFU ml<sup>-1</sup>)  
153 as a function of dose, and are presented as mean values from triplicate independent  
154 experiments (n=3). Dose ( $\text{J cm}^{-2}$ ) is calculated as the product of the irradiance ( $\text{W cm}^{-2}$ )  
155 multiplied by the exposure time (sec), with the irradiance value being the maximum  
156 measured at the centre position of the sample dish/bag. Significant differences in the results  
157 were identified using 95% confidence intervals and one-way analysis of variance (ANOVA)  
158 with Minitab software Release 16. For dose response curves the dose that reduces the  $\log_{10}$   
159 CFU count at 0-dose by 50% was estimated. This 50%  $\log_{10}$  reduction was estimated using



160 curve fitting software (GraphPad Prism V6) and quadratic or 5PL variable slope sigmoidal  
161 curves with R-squared fits in excess of 90%.

162 **Optical Analysis of Plasma:** The transmission values for rabbit and human plasma, PBS,  
163 and the blood bag material, were measured by using a Biomate 5 UV-Visible  
164 Spectrophotometer (Thermo Spectronic). Analysis was carried out in the wavelength range  
165 220-700 nm. Fluorescence spectrophotometry (RF-5301 PC spectrofluorophotometre;  
166 Shimadzu, US) was used to determine whether plasma or PBS contained photosensitive  
167 components which could be excited by 405 nm light. Excitation was carried out at 405 nm  
168 and emission spectra were recorded between 500-700 nm.

169

## 170 **RESULTS**

171 **Inactivation of Microbial Contaminants in 3 ml PBS and Plasma:** Results from the  
172 exposure of PBS, rabbit plasma and human plasma seeded with bacterial contamination  
173 ( $10^5$  CFUml<sup>-1</sup>) to 100 mWcm<sup>-2</sup> 405nm light, are presented in Figure 1. Results demonstrate  
174 that bacterial inactivation in PBS is achieved using the lowest dose. Data for *S. aureus*  
175 (Fig.1a) shows that near complete inactivation (<10 CFUml<sup>-1</sup> surviving) of the organism in  
176 PBS was achieved after exposure to a dose of 60 Jcm<sup>-2</sup>. To achieve a comparable reduction  
177 in rabbit and human plasma, 4.5 times the dose was required (270 Jcm<sup>-2</sup> compared to 60 Jcm<sup>-2</sup>).  
178 50% log<sub>10</sub> reductions were estimated to occur at doses 23, 224 and 181 Jcm<sup>-2</sup> for PBS,  
179 rabbit and human plasma, respectively.

180 Similar inactivation kinetics were observed for *S. epidermidis* (Fig.1b), although this species  
181 showed comparatively greater susceptibility to 405 nm light when exposed in plasma. The  
182 50% log<sub>10</sub> reductions were obtained in PBS, rabbit and human plasma at 36, 121 and 174

183  $\text{Jcm}^{-2}$  respectively. Reduction of *E. coli* contamination required markedly increased doses  
184 (Fig.1c). The 50%  $\log_{10}$  reductions required doses of 328, 585 and 742  $\text{Jcm}^{-2}$  for PBS, rabbit  
185 and human serum respectively. For inactivation in PBS, 450  $\text{Jcm}^{-2}$  was required for near  
186 complete inactivation ( $<10 \text{ CFUml}^{-1}$  surviving): 7.5 times more than observed with the  
187 staphylococci. Inactivation of *E. coli* contamination in plasma again required increased doses  
188 compared to when suspended in PBS, with a 5- $\log_{10}$  reduction in human plasma achieved  
189 after a dose of 1.08  $\text{kJcm}^{-2}$ .

190

191 **Determination of Light Induced Toxicity within Human Plasma:** No significant change in  
192 the seeded  $10^3 \text{ CFUml}^{-1}$  population [ $P=0.663$ ] was evident in the bacterial contamination  
193 added to plasma post-exposure, thus indicating no residual toxicity in 405-nm light exposed  
194 plasma that could induce the inactivation of microbial contaminants.

195

196 **Inactivation of Contaminants in Larger Volumes of Human Plasma:**

197 **30 ml Volume in Covered Sample Dish:** Figure 2 demonstrates the inactivation of  
198 low density *S. aureus* contamination in 30 ml plasma in a closed Petri dish using an  
199 irradiance of  $\sim 8 \text{ mWcm}^{-2}$ . Results for a seeding density of  $10^3 \text{ CFUml}^{-1}$  (Fig 2b) demonstrate  
200 that exposure to doses of greater than 100.8  $\text{Jcm}^{-2}$  caused significant inactivation of the  
201 contamination [ $P=0.030$ ], with near-complete inactivation achieved with 230.4  $\text{Jcm}^{-2}$ .  
202 Control contamination levels rose significantly by approximately 1- $\log_{10}$  over the course of  
203 the experiment [ $P=<0.001$ ]. Similar results were observed for inactivation of the  $10^2 \text{ CFUml}^{-1}$   
204 contamination levels (Fig 2c): significant inactivation became evident after exposure to a  
205 dose of 115.2  $\text{Jcm}^{-2}$  [ $P=0.009$ ], with near complete inactivation achieved with 187.2–

206 230.4 Jcm<sup>-2</sup>. Control contamination levels remained relatively unchanged [P=0.255].  
207 Significant inactivation of a 10<sup>1</sup> CFUml<sup>-1</sup> seeding population was shown after a dose of  
208 115.2 Jcm<sup>-2</sup> [P=0.031], with near complete inactivation achieved by exposure to doses of  
209 201.6-230.4 Jcm<sup>-2</sup> (Fig 2d). Control contamination levels showed no significant change  
210 compared to the exposed samples [P=0.054].

211 **Decontamination of Plasma in a Blood Bag:** Inactivation of low density (10<sup>1</sup>-  
212 10<sup>2</sup> CFU ml<sup>-1</sup>) bacterial contaminants within plasma transfusion bags was achieved using  
213 irradiances as low as 5 mWcm<sup>-2</sup> (Fig.3b) A notable downward trend in contamination was  
214 observed after exposure to 108 Jcm<sup>-2</sup>, with a significant 0.6 log<sub>10</sub> reduction in contamination  
215 [P=<0.001]. Complete/near complete inactivation was achieved after exposure to 144 Jcm<sup>-2</sup>  
216 [P=0.017] This slightly reduced inactivation rate, compared to that found within the sample  
217 dishes, is due to the lower irradiance light being used for exposure. Contamination levels in  
218 the control plasma bags rose by approximately 0.5-log<sub>10</sub> [P=0.052]. Similar inactivation  
219 kinetics were obtained for seeded transfusion bags exposed to irradiances of 16 and  
220 48 mWcm<sup>-2</sup>, with contamination levels decreasing upon exposure to increasing treatment.  
221 Comparison of the results for the three irradiance levels used, demonstrated that, when  
222 looking at exposure time (Fig. 4a), the decontamination effect observed with 16 and  
223 48 mWcm<sup>-2</sup> is relatively comparable, with inactivation being slightly slower when using the  
224 lowest irradiance of 5 mWcm<sup>-2</sup>. However, when looking at the actual dose levels applied  
225 (Figure 4b), it is apparent that the germicidal efficiency (defined as the log<sub>10</sub> reduction of a  
226 bacterial population [log<sub>10</sub>(N/N<sub>0</sub>)] by inactivation per unit dose in Jcm<sup>-2</sup> [23]) of the 5 mWcm<sup>-2</sup>  
227 irradiance is greater than that of the 16 and 48 mWcm<sup>-2</sup> irradiances (P=0.007 and 0.013,  
228 respectively). Comparison of exposure to doses in the region of 140-180 Jcm<sup>-2</sup> highlights this  
229 difference in efficacy, with a 1.91 log<sub>10</sub> reduction being achieved after exposure to 5 mWcm<sup>-2</sup>

230 for 8h ( $144 \text{ Jcm}^{-2}$ ), a  $1.14 \log_{10}$  reduction with  $16 \text{ mWcm}^{-2}$  for 3h ( $172.8 \text{ Jcm}^{-2}$ ), but only  
231  $0.08 \log_{10}$  reduction observed after 1h exposure to  $48 \text{ mWcm}^{-2}$  ( $172.8 \text{ Jcm}^{-2}$ ).

232 **Optical Analysis of Plasma:** Spectrophotometric analysis shows that transmission of  
233 405 nm light through plasma is low (1-2%) compared with transparent PBS (99%), and this  
234 correlates with the longer exposure times/increased doses required for comparative microbial  
235 inactivation in plasma compared to PBS. Figure 5a highlights the transmissibility of the Petri  
236 dish material and the blood bag, with results showing that 405 nm light can transmit through  
237 these materials, thus permitting decontamination of the blood plasma whilst contained in the  
238 sample dish and blood bag. The fluorescence emission spectra of rabbit and human plasma,  
239 and PBS demonstrated that excitation of the suspensions at 405 nm produced no prominent  
240 fluorescence emission peaks between 500 and 700 nm (Fig 5b).

241

## 242 **DISCUSSION**

243 In order to assess the potential of 405 nm light for decontamination of blood plasma, the  
244 penetrability and antimicrobial efficacy of 405 nm light in plasma required evaluation, and  
245 the aim of this study was to determine the antibacterial effects of 405 nm light at varying  
246 irradiances on bacteria seeded in blood plasma ranging from small volume samples up to pre-  
247 bagged plasma.

248 Initial investigation of the inactivation of bacterial contaminants in low volume (3 ml) plasma  
249 samples using  $100 \text{ mWcm}^{-2}$  405 nm light demonstrated that successful inactivation could be  
250 achieved in both rabbit and human plasma. Significantly greater doses were required for  
251 inactivation of bacterial contaminants when suspended in plasma compared to PBS, and this  
252 is accredited to the differing optical properties of these suspending media. The opacity, and

253 consequent low transmissibility of plasma (Fig.5a), reduces photon penetration through the  
254 suspension, resulting in the requirement for greater doses, compared with suspension in clear,  
255 transparent liquids such as PBS. Despite this, these proof-of-principle results demonstrate  
256 that significant inactivation of bacterial contaminants in human plasma can be achieved, with  
257 the higher the irradiance of light applied, the shorter the exposure time required for successful  
258 inactivation.

259 Despite the optical transmission properties of rabbit and human plasma being relatively  
260 similar, slight differences were recorded between the susceptibility of the bacterial  
261 contaminants when seeded in these media. This is likely due to the batch-to-batch variation  
262 in color and opacity of the rabbit and, in particular, the human plasma. Indeed, optical  
263 analysis of a number of human plasma bag samples (n=30) demonstrated variation in  
264 transmission at 405 nm of between 0.2-25% (Maclean, Anderson, MacGregor, Atreya;  
265 unpublished data). This is likely the reason for the large standard deviation in some of the  
266 data points in the inactivation kinetics for the pre-bagged plasma.

267 The bacterial species used in this study were selected to represent significant contaminants  
268 associated with blood components [3]. Although only three organisms were utilized, the  
269 wide antimicrobial efficacy of 405 nm light has been reported in a number of publications  
270 [20,22,23,25,37]. It is therefore expected that these organisms would also be successfully  
271 inactivated by 405 nm light when suspended in plasma. Typically, Gram-positive bacteria  
272 tend to have greater susceptibility to 405 nm light than Gram-negative bacteria [23], and this  
273 is consistent with the results reported here, with approximately 4-times greater dose required  
274 to inactivate *E. coli* in plasma, compared to the staphylococci. Interestingly, the difference  
275 between the susceptibilities of the staphylococci and *E. coli* was less pronounced when  
276 suspended in plasma compared to in PBS (4 versus 7.5 times the dose required).

277 The initial exposure tests in this study to establish proof-of-principle, utilised low volumes of  
278 plasma seeded with high population densities of bacterial contaminants at a level of  
279  $10^5$  CFUml<sup>-1</sup>. A more realistic scenario involves larger volumes of plasma contaminated with  
280 low microbial densities. Indeed, it has been reported that the levels of naturally-occurring  
281 bacterial contamination in plasma are likely to be as low as 10-100 bacterial cells per product  
282 at the beginning of storage [38]. Accordingly, experiments were scaled up 10 and 100-fold  
283 using larger plasma volumes seeded with bacterial contamination levels down to  $10^1$  CFUml<sup>-1</sup>  
284 <sup>1</sup>, using *S. aureus* as the model organism. Results demonstrated that bacterial contamination  
285 levels, even when less than  $10$  CFUml<sup>-1</sup>, can be significantly reduced in larger volumes of  
286 plasma by exposure to 405 nm light. It was interesting to note that, when using similar  
287 irradiances, the bacterial inactivation rates in the 30 ml and 300 ml samples were very similar  
288 ( $\sim 1.5 \log_{10}$  reductions with a dose of  $144 \text{ Jcm}^{-2}$  – Fig.2c, Fig.3b) despite the 10-fold  
289 difference in sample volume. Although the sample volumes were different, the depth of  
290 plasma was similar ( $\sim 1$ -2 cm in both cases) thus indicating that, when using similar  
291 irradiances, it is the depth of plasma that is likely to influence the light inactivation efficacy,  
292 rather than the overall sample volume. Also, results demonstrated that use of lower  
293 irradiances is likely to be more efficient, both in terms of optical energy and antimicrobial  
294 activity, than higher irradiances. This is possibly due to there being a critical level of photons  
295 that can be involved in the photo-excitation of the bacterial porphyrin molecules, and above  
296 this irradiance level, there is provision of excess photons which, although exposing the cells,  
297 are unable to contribute to the reaction due to there being a limit on the free porphyrin to  
298 photon ratio.

299 In addition to demonstrating efficacy when applied to larger volumes of plasma, these  
300 experiments highlighted that the 405 nm light disinfection effect can be achieved through  
301 transparent packaging. A similar effect was reported in a recent study which highlighted the

302 ability of 405 nm light to decontaminate biofilms on the underside of transparent materials  
303 [39]. The ability of 405 nm light to transmit through the PVC bag layer to treat the plasma is  
304 particularly advantageous as it opens up the possibility for pre-bagged plasma to be treated  
305 immediately prior to storage, without the need for addition of photosensitizers, and/or passing  
306 the plasma through external decontamination systems, which can potentially introduce new  
307 contamination into the plasma products [6]. The transmissibility of 405 nm light is also a  
308 significant advantage over UVC-light, which is blocked by the PVC bag material (Fig.5a).  
309 Measurements in the present study demonstrated that transmission of 405 nm light though the  
310 blood component bag material resulted in an approximate 20% loss in irradiance, however  
311 light irradiance can be increased through the use of higher power light sources in order to  
312 compensate for this loss if required. Future developments would also look to improve the  
313 uniformity of the light systems used to treat the plasma.

314 Published studies have identified microbial endogenous porphyrin molecules as the key  
315 photosensitive targets which initiate the lethal oxidative damage exerted by 405 nm and other  
316 violet light wavelengths [19,33]. Since human blood also contains porphyrins and porphyrin  
317 derivatives, it was important to establish that inactivation by 405 nm light in our study was a  
318 result of the photoexcitation reaction within the microbial contaminants, and not a  
319 consequence of excitation of any photosensitive molecules within the plasma, and this was  
320 evidenced by the absence of antimicrobial toxicity to bacterial contaminants seeded into the  
321 405 nm light-exposed plasma. Qualitative analysis of the rabbit and human plasma also  
322 detected no notable fluorescence emission peaks between 500-700 nm when excited at  
323 405 nm, thus indicating no significant levels of free porphyrins or other photoexcitation  
324 sources within the plasma that might have acted as exogenous photosensitizers for the  
325 inactivation of the microbial contaminants.

326 The 405 nm light doses required in this study for the decontamination of blood plasma have  
327 been in the region of  $158 \text{ Jcm}^{-2}$  and above. These doses are relatively high compared to those  
328 typically required for other light-based methods, and this is due to the higher germicidal  
329 efficacy of UV-light compared to 405 nm light [40], and the involvement of photosensitizing  
330 compounds such as riboflavin, methylene blue and amotosalen, also accelerates the  
331 antimicrobial effects of light, with doses as low as  $6.24 \text{ Jml}^{-1}$  being reported as sufficient for  
332 use [7,41]; significantly lower than the  $83 \text{ Jml}^{-1}$  used in the present study (calculated based on  
333 the  $158 \text{ Jcm}^{-2}$  dose, transfusion bag dimensions and volume). This benefit however is  
334 counterbalanced by the fact that photosensitizers are added to the blood products, and  
335 significant care must be taken to ensure there is no toxicity to the blood components or the  
336 recipient due to the presence of residual photosensitizers [6]. Methods utilizing UV-C light  
337 are currently under development and also demonstrate efficient microbial inactivation [16].  
338 Although not requiring photosensitizers, UV-C is naturally more germicidal than 405 nm  
339 light, however, as mentioned, the limited penetrability of shortwave UV-C radiation means it  
340 is unable to decontaminate plasma packed in blood bags, as evidenced in the present study  
341 using 405 nm light (Fig.4a). The longer wavelength of 405 nm light also confers other  
342 benefits when compared to UV-light, including reduced polymer degradation and increased  
343 human safety [42,43].

344 Due to the absence of cells, solvent/detergent treatment, methylene blue and visible light,  
345 amotosalen and UV-A light, riboflavin and UV, and UV-C light are generally accepted as  
346 suitable for plasma decontamination. This study has generated significant evidence of the  
347 efficacy of 405 nm light for decontamination of blood plasma as a model system to study  
348 injectable biological fluids. Since person-to person variation in the activity of plasma  
349 proteins in healthy individuals is known to be significant, any loss in plasma integrity due to  
350 405 nm light treatment is unlikely to have noticeable clinical impact. Further, since violet-



351 blue light (405 nm) is relatively safer compared to already accepted UV-light based methods  
352 [40], its impact on plasma integrity has the potential to be reduced. Nonetheless, it is  
353 important in future studies to establish what effects are imparted onto plasma proteins when  
354 exposed to antimicrobial levels of 405 nm light relative to UV light exposure.

355

## 356 **CONCLUSIONS**

357 Overall, this study provides the first evidence that 405 nm light has the ability to inactivate  
358 bacterial contamination within biological fluids such as blood plasma. Significant  
359 inactivation of microbial contaminants was achieved in plasma samples of varying volumes  
360 held in different containers including pre-bagged plasma. The penetrability of 405 nm light  
361 and the non-requirement for photosensitizing agents, provide this antimicrobial method with  
362 unique benefits that could support its further development as a potential alternative to UV  
363 light-based systems. Further work is however required, not only to extend the  
364 microbiological data, but also to investigate the compatibility of 405 nm light with plasma  
365 components before its potential for plasma decontamination can be fully assessed. Although  
366 this study has focused on the antimicrobial effects of 405 nm light for the decontamination of  
367 plasma, it will also be of interest to establish whether bacterial reductions can be achieved in  
368 platelets stored ex vivo in plasma-based suspensions, which have a significantly greater risk  
369 of contamination due to the limitations of their storage conditions.

370

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379 Scottish National Blood Transfusion Service (SNBTS) for provision of blood components.

380

### 381 **CONFLICT OF INTEREST**

382 The authors declare that there is no conflict of interest regarding the publication of this paper.  
383 The authors have filed a joint US device patent application.

384

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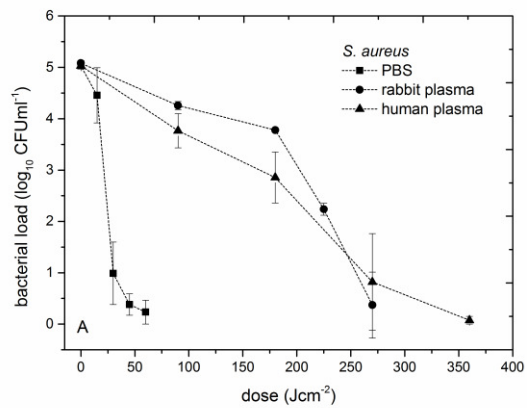
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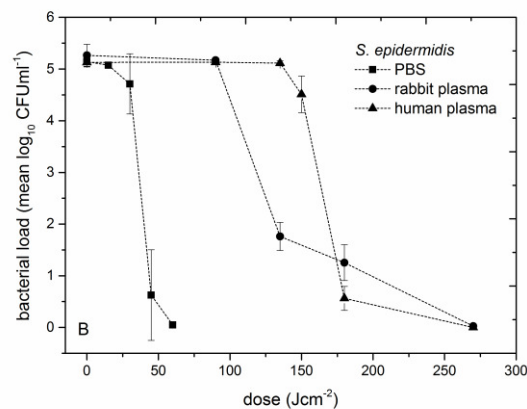
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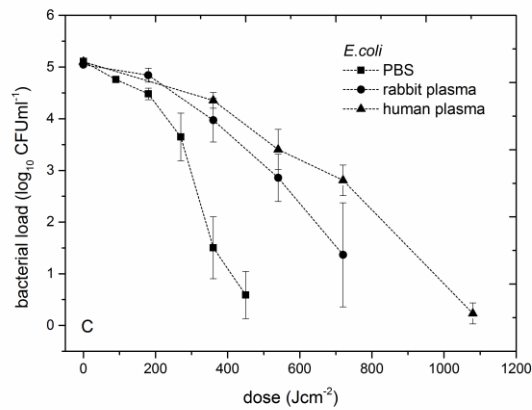




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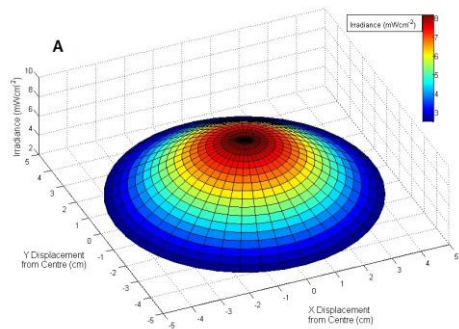


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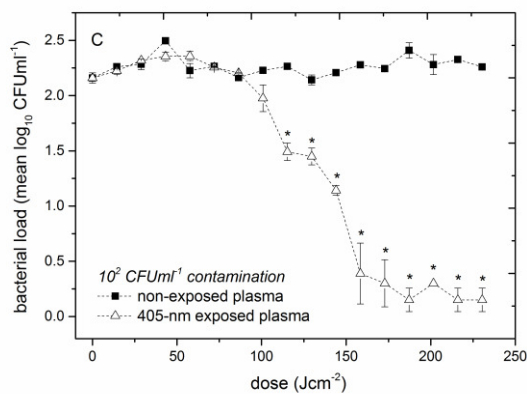
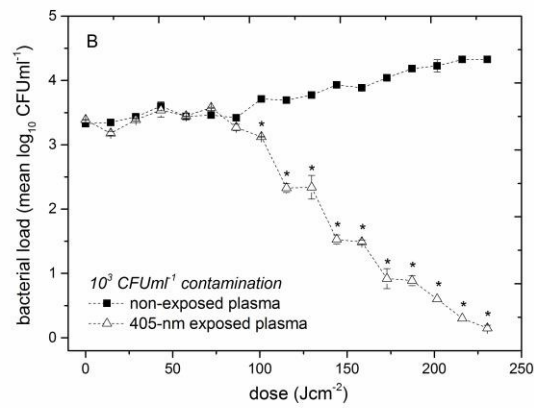


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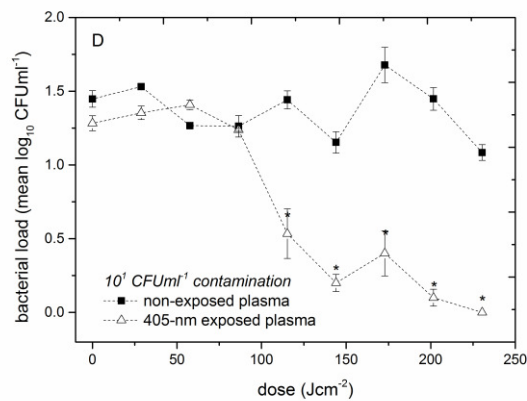
531 **Fig 1:** Inactivation of bacterial contamination, (a) *S. aureus*, (b) *S. epidermidis* (c) *E. coli*, in  
 532 phosphate buffered saline (PBS) rabbit plasma, and human plasma, by exposure to 405 nm  
 533 light with an irradiance of approximately 100 mWcm<sup>-2</sup> (n=3 ±SD). Non-exposed control  
 534 samples for all experiments demonstrated no significant change in population over the  
 535 exposure period [P=>0.05].



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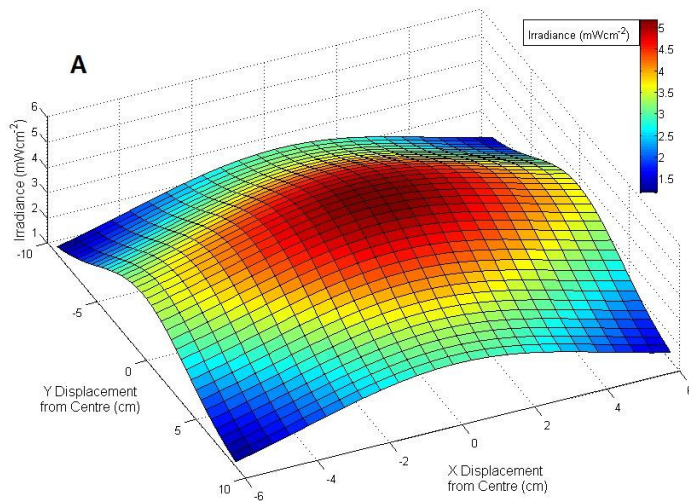


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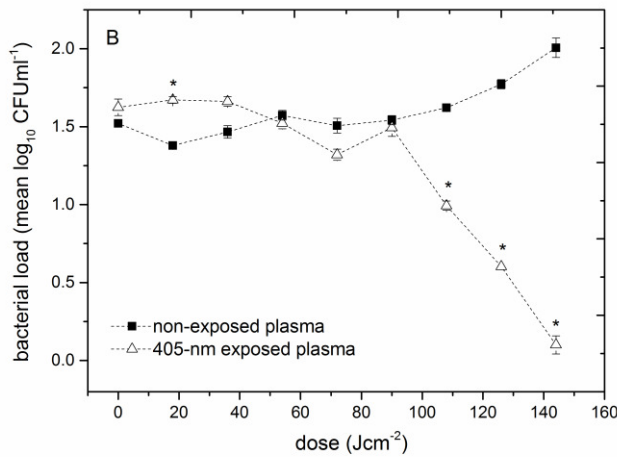


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539 **Fig 2:** Inactivation of *S. aureus* contamination in 30 ml volumes of human plasma held in a  
 540 closed sample dish by exposure to 405 nm light. (a) Three-dimensional model demonstrating  
 541 the irradiance profile across the sample dish, with an irradiance of  $\sim 8 \text{ mWcm}^{-2}$  at the centre.  
 542 Populations of (b)  $10^3$ , (c)  $10^2$  and (d)  $10^1 \text{ CFUml}^{-1}$  were used as the seeding densities ( $n=3$   
 543  $\pm \text{SE}$ ). Asterisks (\*) represent data points where the bacterial levels in light-exposed plasma  
 544 were significantly different to the equivalent non-exposed control [ $P < 0.05$ ].



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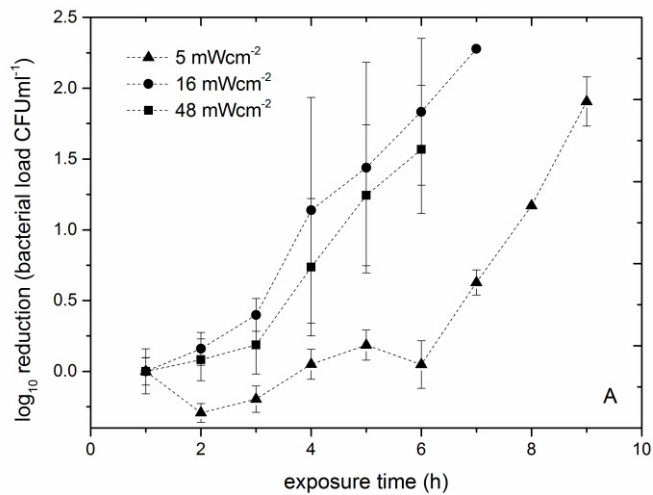


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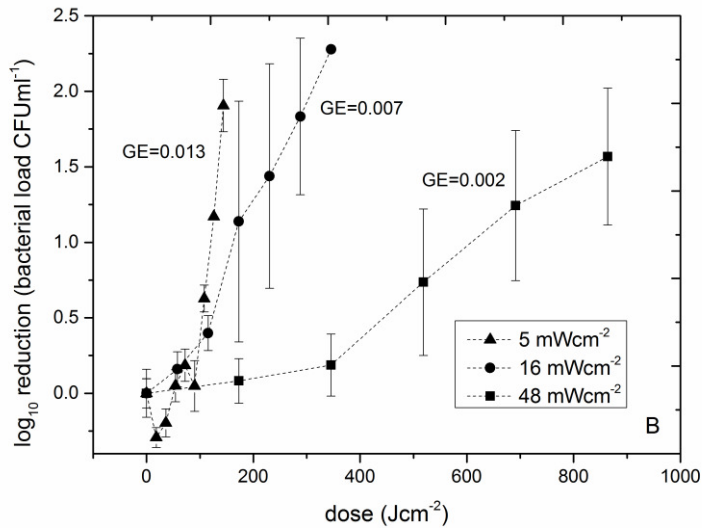
547

548 **Fig 3:** 405 nm light exposure of contaminated human plasma transfusion bags (a) Three-  
 549 dimensional model demonstrating the irradiance profile across the plasma bag, with an  
 550 irradiance of  $\sim 5 \text{ mWcm}^{-2}$  at the centre (b) Inactivation of *S. aureus* contamination in 300 ml  
 551 bags of human plasma by exposure to 405 nm light ( $n=3 \pm \text{SE}$ ). Asterisks (\*) represent data  
 552 points where the bacterial levels in light-exposed plasma were significantly different to the  
 553 equivalent non-exposed control [ $P < 0.05$ ].

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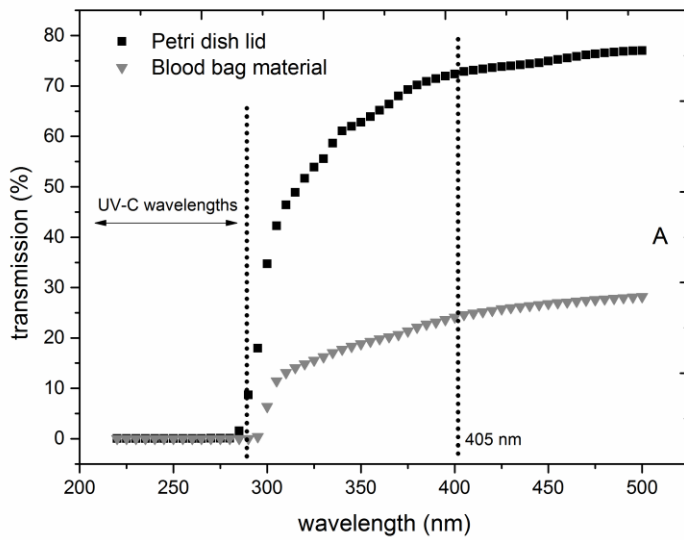


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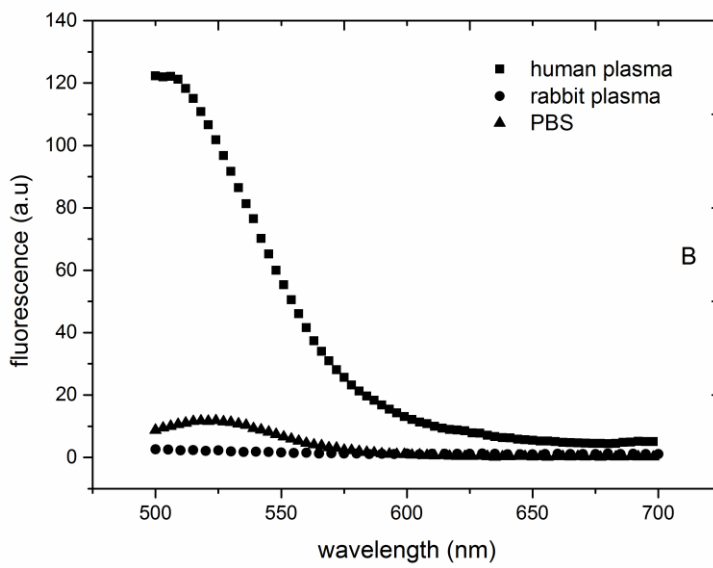


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557 **Fig 4:** Comparison of the exposure times (a) and doses (b) required for inactivation of  
 558 *S. aureus* contamination in human plasma transfusion bags. (a) Inactivation kinetics were  
 559 achieved utilising irradiances of 5, 16 and 48 mWcm<sup>-2</sup> at the centre of the bags. Results are  
 560 presented as log<sub>10</sub> reduction (CFUml<sup>-1</sup>) as compared to the equivalent non-exposed control  
 561 samples (n=3 ±SD). Germicidal efficiency (GE) values for each of the irradiances are shown  
 562 on (b). (GE is defined as the log<sub>10</sub> reduction of a bacterial population [ $\log_{10}(N/N_0)$ ] by  
 563 inactivation per unit dose in Jcm<sup>-2</sup>).



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565

566 **Fig 5:** Optical analysis (a) Transmission properties of the Petri dish and blood bag material,  
 567 highlighting 405 nm and UV-C light wavelengths for reference; (b) Fluorescence emission  
 568 spectra of PBS and plasma (500-700 nm), detected using an excitation wavelength of 405 nm.

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570