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Abstract

Diabetes mellitus (DM) involves metabolic changes that can impair bone repair, including a prolonged inflammatory response. A salicylic acid-based poly(anhydride-ester) (SA-PAE) provides controlled and sustained release of salicylic acid (SA) that locally resolves inflammation. This study investigates the effect of polymer-controlled SA release on bone regeneration in diabetic rats where enhanced inflammation is expected. Fifty-six Sprague–Dawley rats were randomly assigned to two groups: diabetic group induced by streptozotocin (STZ) injection or normoglycemic controls injected with citrate buffer alone. Three weeks after hyperglycemia development or vehicle injection, 5 mm critical sized defects were created at the rat mandibular angle and treated with SA-PAE/bone graft mixture or bone graft alone. Rats were euthanized 4 and 12 weeks after surgery, then bone fill percentage in the defect region was assessed by micro-computed tomography (CT) and histomorphometry. It was observed that bone fill increased significantly at 4 and 12 weeks in SA-PAE/bone graft-treated diabetic rats compared to diabetic rats receiving bone graft alone. Accelerated bone formation in normoglycemic rats caused by SA-PAE/ bone graft treatment was observed at 4 weeks but not at 12 weeks. This study shows that treatment with SA-PAE enhances bone regeneration in diabetic rats and accelerates bone regeneration in normoglycemic animals.

Keywords

poly(anhydride-ester, salicylic acid, diabetes, bone regeneration

Disciplines

Endocrinology, Diabetes, and Metabolism | Osteopathic Medicine and Osteopathy

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Locally Delivered Salicylic Acid from a Poly(anhydride-ester): Impact on Diabetic Bone Regeneration

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Abstract

Diabetes mellitus (DM) involves metabolic changes that can impair bone repair, including a prolonged inflammatory response. A salicylic acid-based poly(anhydride-ester) (SA-PAE) provides controlled and sustained release of salicylic acid (SA) that locally resolves inflammation. This study investigates the effect of polymer-controlled SA release on bone regeneration in diabetic rats where enhanced inflammation is expected. Fifty-six Sprague-Dawley rats were randomly assigned to two groups: diabetic group induced by streptozotocin (STZ) injection or normoglycemic controls injected with citrate buffer alone. Three weeks after hyperglycemia development or vehicle injection, 5 mm critical sized defects were created at the rat mandibular angle and treated with SA-PAE/bone graft mixture or bone graft alone. Rats were euthanized 4 and 12 weeks after surgery, then bone fill percentage in the defect region was assessed by microcomputed tomography (CT) and histomorphometry. It was observed that bone fill increased significantly at 4 and 12 weeks in SA-PAE/bone graft-treated diabetic rats compared to diabetic rats receiving bone graft alone. Accelerated bone formation in normoglycemic rats caused by SA-PAE/bone graft treatment was observed at 4 weeks but not at 12 weeks. This study shows that treatment with SA-PAE enhances bone regeneration in diabetic rats and accelerates bone regeneration in normoglycemic animals.

Keywords

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1. Introduction

Diabetes mellitus (DM) is a common metabolic disorder associated with hyperglycemia and hyperlipidemia due to lack of insulin or insulin resistance and affecting 8.3 % of the U.S. population in 2011 [1]. DM has been shown to increase systemic inflammation and prolong inflammatory response to injury [2]. Specifically, DM enhances inflammation through the formation of reactive oxygen species, advanced glycation endproducts, hypoinsulinemia, and/or insulin resistance [3].

Type 1 diabetes causes osteopenia, and both type-1 and type-2 diabetes have been linked to poor bone quality and reduced capacity to form bone [4–5]. Factors contributing to this deficit include decreased transcription factor expression needed to regenerate bone [6], inflammation [7], and diminished vascularity [8]. Furthermore, diabetes-enhanced inflammation has been linked to prolonged osteoclastogenesis that may reduce bone quality [9–11].

Bone grafting is often used to treat orthopedic and oral-facial defects [12–13]. In DM, however, bone regeneration procedures result in a greater degree of variability and increased infection rates [14–15]. Growth factors have been extensively studied and found to be beneficial for bone regeneration in humans [16–17]. However, they are extremely expensive and some still have unresolved safety concerns (e.g., high complication rates and potential carcinogenicity of bone morphogenetic proteins (BMPs) in human [18–19]). As a result, exploring new methods to improve bone regeneration is necessary, especially in diabetic subjects whose bone regeneration capability is compromised by long term diabetes-enhanced inflammation.

Salicylic acid-based poly(anhydride-esters) (SA-PAE) have been synthesized by chemically incorporating salicylic acid (SA) within a polyanhydride [20]. SA-PAEs degrade via hydrolysis of anhydride and ester bonds and release SA and a biocompatible molecule, in our case adipic acid (Figure 1) [21–22]. SA is an anti-inflammatory that reduces the production of pro-inflammatory cytokines such as prostaglandins, TNF- α , IL-1, and IL-6 [23]. Several studies have shown that elevation of these cytokines impairs bone healing by affecting the activity and survival of osteoblasts and osteoclasts [24–27]. Therefore, SA-PAEs could potentially improve bone regeneration through mediation of inflammation.

In this study, the influence of localized, sustained delivery of SA on bone regeneration in diabetic and normoglycemic rats was evaluated. Our results indicate that SA delivered by an SA-PAE significantly promotes new bone formation in diabetic rats and accelerates new bone formation in normoglycemic rats.

2. Material and Methods

2.1. Sample Preparation

The SA-PAE was synthesized using previously reported methods [28]. The polymer was ground into a fine powder and physically mixed with freeze-dried bone allograft (LifeNet Health®, Virginia Beach, VA) at a 1:1 weight ratio (7.5 mg of SA-PAE mixed with 7.5 mg of bone graft). Approximately 40 μ L light mineral oil (Sigma-Aldrich, Milwaukee) was added to the mixture, which was then sterilized under ultra-violet light in a Spectrolinker XL-1500 UV Crosslinker (Spectronics Corporation, Westbury, NY) at λ = 254 nm and 5,500–6,500 μ W/cm² for 900 s. Control samples were prepared without SA-PAE and treated identically to the SA-PAE-containing samples.

2.2. In Vitro SA-PAE/Bone Graft

The SA release from samples prepared in section 2.1 was evaluated *in vitro* using phosphate buffered saline (PBS) (Sigma-Aldrich, Milwaukee). PBS pH was adjusted to 7.4 using 1 N sodium hydroxide. All pH measurements were performed using an Accumet® AR15 pH meter (Fisher Scientific, Fair Lawn, NJ). To measure SA release, 15 mg of sterilized samples (n=3) were placed in 20 mL Wheaton glass scintillation vials with 10 mL of PBS and incubated at 37 °C with agitation at 60 rpm using a controlled environment incubator-shaker (New Brunswick Scientific Co., Edison, NJ) to mimic physiological conditions. The buffer solution was replaced with fresh PBS (10 mL) every 24 hours and analyzed over 21 days. Spent media was analyzed by UV spectrophotometry using a Perkin Elmer Lambda XLS spectrophotometer (Waltham, MA) to specifically monitor SA release. Measurements were obtained at $\lambda = 303$ nm, the maximum absorbance of SA that does not overlap with other polymer degradation products. Data were calculated against a calibration curve of absorbance values from standard solutions of known SA concentrations in PBS.

2.3. Animal Model

Animal care and surgical procedures were approved by the IACUC of the University of Pennsylvania. Fifty-six adult male Sprague-Dawley rats weighing 250 g – 350 g were used, n= 7 per group. The rats were randomly divided into diabetic and normoglycemic groups. Diabetes was induced by intraperitoneal injection of streptozotocin, 70 mg/kg (Sigma-Aldrich, Milwaukee, WI). Blood glucose was monitored by the glucose-oxidase method (Glucometer Encore, Miles, Elkhart, IN) and HbA1c was measured at the time of euthanasia (Table 1). A blood glucose level greater than 250 mg/dL was considered diabetic. Animals were monitored for 3 weeks to confirm their diabetic status and to evaluate their daily food intake, activity, weight, and overall health. Of the 56 rats that underwent surgery, two died during the procedure; no significant reductions in body weight occurred and 3 postoperative infections were observed in the diabetic group.

2.3.1. Surgical Procedure—All procedures were performed under general anesthesia with an intraperitoneal injection of ketamine, 75 mg/kg (Fort Dodge Laboratories, Fort Dodge, IA) and xylazine, 5 mg/kg (Miles Inc., Shawnee Mission, KS). Surgical procedures were performed under sterile conditions. A 15 to 20 mm incision was made on the lateral aspect of the mandible. A 5 mm diameter osteotomy defect was created at the angle of the mandible using a trephine burr with sterile saline irrigation. The site was grafted with SA-PAE/bone graft mixture or bone graft alone, as prepared in section 2.1. A BioGuide® resorbable collagen membrane (Geistlich Pharma., North America Inc., NJ) was adapted to circumferentially cover the defect. The surgical field was closed in layers, a muscular layer and the external skin layer, using Chromic gut 5-0 resorbable sutures (Ethicon, Somerville, NJ). A single dose of buprenorphine (0.05 mg/kg) was administered for postoperative pain relief. Rats were euthanized at 4 and 12 weeks. The mandibles were dissected and fixed in 4% phosphate buffered formalin solution for 24 hours and then stored in PBS until microcomputed tomography (micro-CT) scans were performed.

2.4. Micro-Computed Tomography

Micro-CT images were obtained using a eXplore Locus SP micro-CT scanner (GE Healthcare, Pittsburgh, PA). Images were taken at a resolution of 48 µm. The micro-CT data sets were reconstructed with the GEHC eXplore Scan Control (GE Healthcare, Pittsburgh, PA) and evaluated by OsiriX 64 image analysis software (Pixmeo, Geneva, Switzerland). The original circular defect was located, and a 3-D region-of-interest (ROI) measuring 5.0 mm in diameter and 0.3 mm in height was established for the original defect. A bone/no-bone threshold value in CT Hounsfield units (HU) was determined and used to measure the

mineralized bone (new bone and bone graft) present in the osteotomy defect. For each specimen, new bone formation was expressed as a percentage of mineralized bone in the 5.0 mm diameter defect. The number of samples per group was 6 to 7.

2.5. Histologic Analysis

After micro-CT scan, specimens were demineralized with 10% EDTA (Fisher scientific USA, Pittsburgh, PA), which was changed three times per week for 7 weeks. The specimen was cut in half after decalcification, embedded in paraffin and sectioned at the midline of the defect. 5 µm thickness histologic sections were prepared and stained with hematoxylin and eosin. Histologic analysis was performed using NIS Elements software (Nikon, Melville, NY) and the percentage of new bone in the defect area was assessed. One half of the defect was analyzed and the percentage of new bone formation was calculated by dividing the area of new bone within the defect on one side by the total area of that side (2.5 mm in length). Some samples were lost due to technical reasons. The number of samples per group was 3 to 4.

2.6. Statistical Analyses

Data are presented as mean \pm standard deviation (SD) or mean + SD. The difference between diabetic and normoglycemic groups at each time point was analyzed by Student's t-test. Significance was determined at p < 0.05.

3. Results

3.1. In Vitro SA Release from SA

The formulation described herein includes bone graft, mineral oil and SA-PAE. To test whether the addition of bone graft and mineral oil influenced SA release rates, an *in vitro* study was performed in PBS over 21 days using this new formulation and analyzed by UV spectrophotometry to ascertain the release profile. The normalized, cumulative SA release curves (Figure 2), demonstrates that SA was released after a lag period of minimal to no SA (2 days). Near zero-order release, common for polyanhydrides and poly(anhydride-esters) due to their surface-eroding behavior [29–30], was observed from days 3–13. These results demonstrate that this new formulation sustained SA release over 16 days.

3.2. Bone Fill of Osteotomy Defect

The amount of mineralized bone (new bone and bone graft) in the osteotomy defect was measured by micro-CT (Figure 3). At the 4-week time point (Figure 4), SA-PAE/bone graft-treated rats had significantly higher bone fill percentage than the control rats (bone graft only) (p < 0.05). Specifically, diabetic rats treated with SA-PAE/bone graft had 44% more bone fill than diabetic control rats (bone graft only), and normoglycemic rats treated with SA-PAE/bone graft bone graft had 37% more bone fill than normoglycemic control rats (bone graft only).

At 12 weeks (Figure 4), diabetic rats treated with SA-PAE/bone graft had 43% more bone fill than the diabetic control rats (bone graft alone) (p < 0.05). No significant difference in bone fill percentage was observed between normoglycemic rats receiving SA-PAE/bone graft and the controls (bone graft alone) (p > 0.05). The percentage of bone fill normoglycemic control group was 32% greater than the diabetic control group (p < 0.05). However, no significant difference in bone fill percentage was observed between the SA-PAE/bone graft-treated group and the control group in normoglycemic rats.

3.3. Histologic Analysis

Results from histologic analysis at 12 weeks agree with the micro-CT results (Figure 5 and 6). Treatment of diabetic rats with SA-PAE/bone graft resulted in 115% more bone fill than diabetic control rats (p < 0.05), whereas treating normoglycemic rats with SA-PAE/bone graft did not increase bone fill significantly (p > 0.05). In additon, bone fill percentage in the normoglycemic control group was 101% greater than the diabetic control group (p > 0.05).

4. Discussion

Our results demonstrate the positive effect of localized, controlled, and sustained SA release on bone regeneration in both diabetic and normoglycemic rats. It significantly enhanced bone regeneration of diabetic rats at 4 and 12 weeks and normoglycemic rats at 4 weeks (Figure 4, 6). One explanation for this positive result centers on the sustained SA release from SA-PAE; SA suppresses nuclear factor kappa-light-chain-enhancer of activated B cells (NF-kB) activation and thus reduces the production of pro-inflammatory cytokines, such as IL-1, IL-6, and TNF- α [31]. These cytokines have been reported to reduce bone formation and enhance bone resorption so their down-regulation by SA would favor bone regeneration [32]. Further, the SA COX inhibiting effect reduces prostaglandin production, which could reduce bone resorption [33–35]. Yet, other studies have also reported that prostaglandin can increase bone formation [36]. The mechanism determining the anabolic or catabolic effect of prostaglandin on bone formation is still unknown [37].

Another explanation for SA-PAE enhanced bone formation is the controlled SA release from SA-PAE; specifically, a lag period followed by sustained SA release. The lag period (i.e., minimum-to-no SA release) allows the initial inflammatory response to develop, which is necessary for subsequent bone healing to occur [38]. After the lag period, sustained SA release resolves prolonged inflammation and thus favors bone regeneration, as suggested by previous studies [39–40]. Our results show that the SA-PAE has greater effects on diabetic rats than normoglycemic rats at the 12-week time point. This is potentially due to the diabetes-enhanced long-term inflammation that impairs bone regeneration, which agrees with the significantly lower bone regeneration in diabetic rats compared to normoglycemic rats at 12 weeks (Figure 4, 6). Therefore, the SA anti-inflammatory effects could lead to a greater difference between the experimental group and the controls in diabetic rats.

Our results agree with previous work where SA-PAEs increased bone formation *in vivo* in normoglycemic animals [40]. A previous study using a localized SA-PAE implantation, however, did not increase bone formation [41]. The difference is potentially due to a much lower SA-PAE dosing used herein (about 17 times less SA-PAE compared to the previous study) and different formulation (i.e. combining SA-PAE with bone graft and mineral oil). These factors may render a higher level of initial inflammation that is desirable for subsequent healing. Compared to other studies evaluating nonsteroidal anti-inflammatory drugs (NSAIDs) effects on bone regeneration, whose results suggest that NSAIDs do not favor bone regeneration [42], our results show a positive effect of SA. The difference in findings is likely caused by our unique drug delivery system that releases SA in a localized, controlled, and sustained manner. Another factor contributing to the positive SA-PAE effect observed is the diabetic condition of animals, for which anti-inflammatory treatments are expected to be more beneficial due to the long-term diabetes-enhanced inflammation.

5. Conclusion

Treatment with SA-PAE/bone graft enhances bone regeneration in diabetic rats and accelerates bone regeneration in normoglycemic animals. This study is the first time that an SA-PAE has been applied to diabetic animals for bone regeneration purposes; our results

suggest that a mixture of SA-PAE/bone graft is very effective on diabetic bone healing. In addition to the advantages of localized, controlled and sustained SA release, our polymer system enables the incorporation of other bioactives (such as insulin) to further improve bone regeneration. Future studies will focus on the mechanism of SA-PAE-enhanced diabetic bone regeneration and incorporating other bioactives into the polymer matrix to improve system performance.

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Figure 1. SA-PAE degradation releases SA and adipic acid upon anhydride and ester bond hydrolysis.







Figure 3.

Representative micro-CT images of mineralized bone formation in defect region (gray circle). Diabetic (A, C, E, G) and normoglycemic (B, D, F, H) rats were implanted with SA-PAE/bone graft (A, B, C, D) or bone graft alone (E, F, G, H) in the 5mm diameter critical size defect. N=6-7/group. Bar = 1 mm.



Figure 4.

Quantitative comparison in mineralized bone (new bone and bone graft) within the defect analyzed by micro-CT. Data are presented as mean + standard deviation. N = 6-7/group. (*p < 0.05).



Diabetic

Normoglycemic

Figure 5.

Representative H&E staining of one half of the defect region where new bone formation was quantified at 12-week time point. New bone formed (enclosed by green dotted line) in one half of the defect (enclosed by black dotted line) is marked. Diabetic (A, C) or normoglycemic (B, D) rats implanted with SA-PAE/bone graft (A, B) or bone graft alone (C, D) in the 5 mm diameter critical size defect. N = 3-4/group.



Figure 6.

Histomorphometric comparison of new bone percentage within the defect at 12 weeks. Data are presented as mean + standard deviation (n = 3-4, *p < 0.05).

Table 1

HbA1c levels in streptozotocin induced diabetes (n = 6) (mean \pm standard deviation)

4 weeks	12 weeks
11.76 ± 1.01	10.78 ± 1.16