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**Evaluation and reproducibility of volumetric measurements on
maxillary sinuses.**

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1. Introduction

The maxillary sinus is a triangular pyramid in the body of the maxilla. It presents three recesses: an alveolar recess pointed inferiorly, bounded by the alveolar process of the maxilla; a zygomatic recess pointed laterally, delimited by the zygomatic bone, and an infraorbital recess pointed superiorly, bounded by the inferior orbital surface of the maxilla. The size of sinuses varies in different skulls, and even on the two sides of the same skull. To measure the internal dimension of the maxillary sinus has proven to be a challenge for researchers [1,5]. Considering the complex structure of maxillary sinuses, magnetic resonance imaging (MRI) and x-ray computed tomography (CT) are the gold standard methods to depict the true anatomy of the Highmore's antrum. Nevertheless, their use is limited by high dose, cost, or restricted accessibility [6,7].

These drawbacks were overcome with the introduction of cone-beam computed tomography (CBCT) [6,7]. Using CBCT technology, measurements of the maxillary sinus volume and the quantification of craniofacial structures are now available that reduce radiation dose compared with CT scans as well as reduced costs compared with MRI. CBCT data sets allow the possibility of a realistic representation of the head of the patient and have expanded diagnostic possibilities, enabling three-dimensional (3D) simulation of surgical and orthodontic procedures. In addition, since its introduction in 1998, CBCT technology has also been improved in terms of accuracy in identifying the boundaries of soft tissues and empty spaces (air). Concerning these advantages, CBCT technology became the elective tool in Orthodontics and Maxillofacial surgery when three-dimensional analysis was required. It is now easier to get a CBCT full skull report instead CT or MRI of orthodontics patients.

Image thresholding is the basis for segmentation. When the user determines a threshold interval, it means that all voxels with grey levels inside that interval will be selected to construct the 3D model (segmentation).

Although this advantages, most CT studies only determined the linear metric variables for define the maxillary sinus, conversely, a valid protocol for 3D volume assessment is still required [9,12].

The main obstacle is still the lack of information on the influence of human error on instrumentation, which could cause measurements to deviate from their actual values [14]. Moreover, only a few studies have tested volumetric analysis techniques with a phantom model [15,16]. For these reasons, validation studies to define the experimental uncertainty are decisive in the estimation of volumetric analysis techniques [14].

The aim of our study is to validate the use of Dolphin Imaging software to analyze CBCT images as a tool for volumetric estimation of maxillary sinus volumes and to test the intra- and inter-examiner reproducibility of this technique. In addition, other aims is to demonstrate the absence of correlation between the volumetric dimensions of the paranasal maxillary spaces and the three different skeletal types.

2. Materials and methods

A validation of the method with well-characterized phantoms was conducted to test the experimental procedure in advance.

To evaluate software reliability, we used six known-volume phantoms replicating the geometrically complex anatomy of the maxillary sinuses (Fig.1):

- Three empty glass containers dipped inside a cylinder of alginate (Phase5, Zemach); (Impregum™, 3M Espe, Germany).
- Three empty glass containers dipped inside a cylinder of alginate and partially filled with alginate (Impregum™, 3M Espe, Germany).

These custom-made phantoms with known volumes were used as the gold standard, and their volume was confirmed by using the water weight equivalent. The volume of the glass containers was calculated by filling

them completely with distilled water (1 atm at 20°C). Water weight was determined by using a digital scientific scale (Gibertini TM560, Max 560g d=0,01g). The precision scale was first calibrated by measuring the empty containers. The weight of the distilled water (calculated in grams) was converted in volume (calculated in mm³) using a specific conversion table. Therefore, we dipped the containers inside a cylinder made of alginate to mimic the soft tissue attenuation of x-rays.

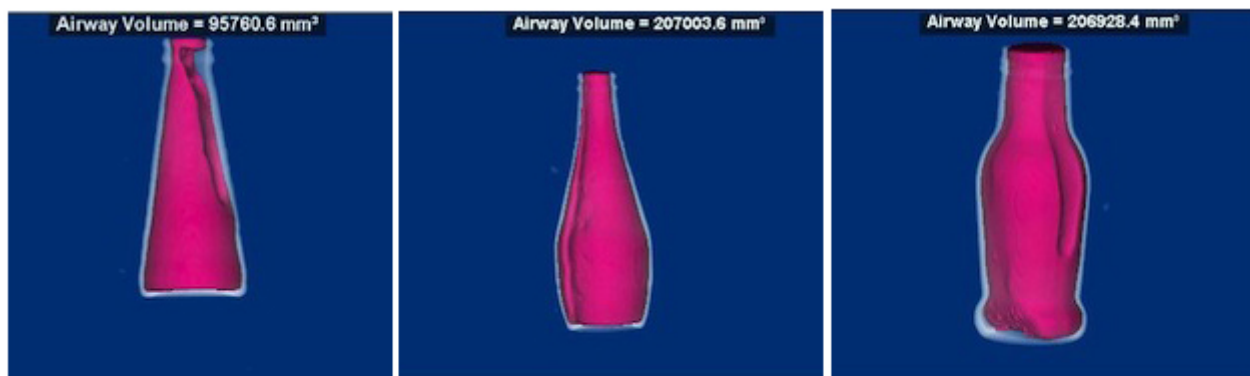


Fig. 1: known-volume phantoms.

Additionally, the 3D scans of 104 maxillary sinuses of a 52 Caucasian adults (mean age 24.3 ± 6.5 years, 26 females and 26 males) was retrospectively examined (Fig 2). All subjects had received a cone beam evaluation of the stomatognathic apparatus for the following reasons: (i) teeth extraction, such

as wisdom teeth; (ii) orthodontic evaluation of unerupted teeth; (iii) the study of cephalometric aspects (lateral and postero-anterior), and (iv) a dental implant.

The exclusion criteria included history of paranasal sinus surgery and maxillofacial trauma, subjects with upper airway pathology, such as clinical sinusitis, and/or cysts of the maxillary sinus and odontogenic cysts, subjects with maxillofacial syndromes. A cephalometric study was conducted on lateral cephalograms obtained from the volumetric 3D data. Subsequently, patients were divided according to Angle's skeletal classifications. SNA, SNB, and ANB angles has been used to assign patients to the appropriate skeletal groups: Skeletal class I ($0^\circ < \text{ANB} < 4^\circ$); Skeletal class II ($\text{ANB} > 4^\circ$), and Skeletal class III ($\text{ANB} < 0^\circ$).

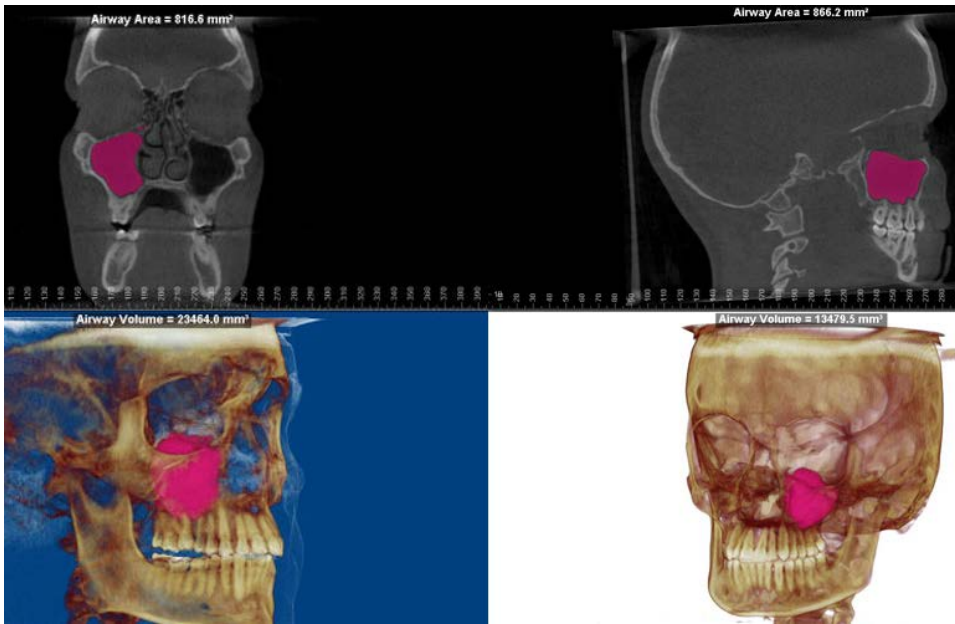


Fig 2: 3D scans of maxillary sinuses, airway area and volume.

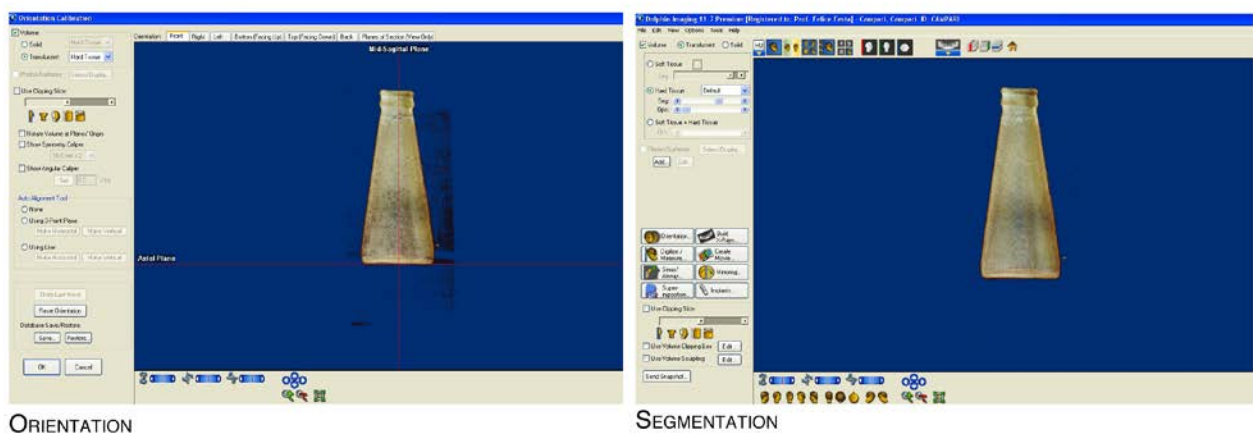
Patients and phantoms were scanned with PAX ZENITH 3D™ Cone beam volumetric tomography (pax zenith 3d vatech SUITE 705A, FORT LEE, NJ), with a reconstructed layer thickness of 0.3 mm and a 512×512 pixel matrix. The device was operated at 120 kVp and 3-8 mA by using a high frequency generator with a fixed anode and a 0.5 mm focal spot. A single 40-s high-resolution scan was made of each skull. The voxel size was set at 0.25 mm, and the images were exported as DICOM files. Each maxillary sinus was visualized in the proper bone density range (1350–1650 gray scale range) and then graphically isolated prior to 3D and volumetric measurements [15].

2.1 Segmentation Procedure

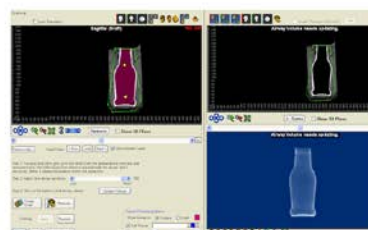
The obtained CT data were analyzed with Dolphin Imaging software (Dolphin Imaging and Management solution, USA). The raw data sets, in DICOM format, were imported in the program 3D Dolphin Imaging. To segment the data correctly, a calibration of the software should be performed following the procedure described below:

- 1) The type of tissue should be set: Hard (hard tissues), Soft (soft tissue), or Soft + Hard tissues (both), depending on the volume imported and of which part you want to examine.
- 2) Radiological artifacts were eliminated, as well as any excess in the volumetric reconstruction; thus a precise portion to be examined were delimited.
- 3) Reorientation of the volume in the three spatial planes was applied, correcting any errors in the positioning of the skull (or phantom) during the CT scan, or simply orienting it in a desired position (see Fig. 3).
- 4) The Sinus/Airway tool function of Dolphin was set as follows:

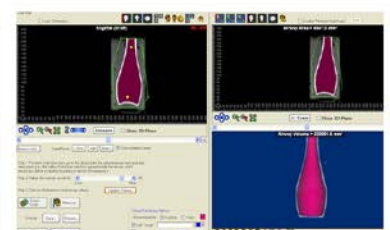
- Step 1: “clipping boundary and seed points”, where the airway structure has been identified selecting boundary points (seed points) in the coronal, axial and sagittal planes.
- Step 2: "slice airway sensitivity", where the sensitivity of the virtual sensor was applied to discriminate airspace. In this study, the "sensitivity tool" was set to a value of 85/100.
- Step 3: "Update volume", where selecting this option the volume was calculated.



AIRWAYS



CLIPPING BOUNDARY AND SEED POINTS



AIRWAY SENSITIVITY AND UPDATE VOLUME

Fig 3: segmentation procedure.

2.2 Measurements

All examiners were trained to use the above standardized study procedure and software tools. They performed phantom measurements in a dark room independently from each other and were blind to previous readings. Each measurement cycle was performed four times with an interval of 60 days between sessions to minimize personal memory effects. All segmentations were evaluated in random order by (A1) one graduate dental student (A2), one well-experienced radiologist (A3), one well-experienced oral surgeon (A4) and one associate professor of Orthodontics. Each phantom was evaluated four times by the single operators.

The error of the method of the maxillary sinuses analysis was then calculated. One operator performed 30 double measurements with an interval period of 30 days. Finally, all measurements on maxillary sinus volumes were assessed (see Fig. 2).

2.3 Data Analysis

Data were analyzed on a personal computer using Excel 2000 (Microsoft Corporation, Redmond, WA, USA) and SPSS 14.0 (SPSS Inc., Chicago, IL, USA) on a Microsoft Windows XP platform.

To assess the repeatability of multiple measurements for each Operator, and to compare the measurements among Operators, RM ANOVA was applied [17].

The Correlation Coefficient (Pearson Product-Moment Correlation Coefficient, r) was calculated to describe the strength of the association between the real and Operator measurements. Each pair of data were plotted and a line of equality was plotted.

Additionally, the method described by Bland and Altman was applied to assess the agreement between target measurements and those of each Operator [17].

The most straightforward measure of disagreement between the two observations is simply the difference between the real measurements and those of each Operator; the mean difference (d) is a measure of the bias and the standard deviation (s) is a measure of the variation between the two

observations. The difference against the mean between the target and Operator measurements was plotted.

To analyze the error of the method, a non-parametric Kolmogorov-Smirnov test (KS test) and a parametric test (T-test) were performed. Before running the T-test, the normality hypothesis and the equal variance hypothesis were tested. The Student's T test was applied to compare right and left sinuses in the skeletal classes' groups.

RM ANOVA was applied, independently from the skeletal groups division, to compare between them i) all the sinuses' volumes, ii) all the right sinus volumes, iii) all the left sinuses volumes.

A Mann-Whitney Sum rank test was applied to investigate the differences between male and female sinus volumes.

3.Results

The RM ANOVA results demonstrated the repeatability of the measurement for each Operator, confirming that the variability among observations isn't statistically significant. No statistically significant differences were observed among Operators, confirming the reliability of the method, independently from the Operator (Table 1).

Statistical significance (P= 0,05) of comparisons among multiple measurements for each Operator and among Operators (RM Anova)

Real measurements	P = 0,2
Operator 1 measurements	P = 0,3
Operator 2 measurements	P = 0,2
Operator 3 measurements	P = 0,8
Operator 4 measurements	P = 0,08
Operators 1, 2, 3, 4	P = 0,1

Table 1: RM Anova results: comparisons among multiple measurements for each Operator and among Operators.

The Correlation Coefficient (Pearson Product-Moment Correlation Coefficient, r) demonstrated a strength association between real measurement and that of each Operator ($r = 1$).

The plot of the difference against the mean between the target measurements and the measurements of each Operator is shown in Figures 4-7.

The mean difference (d) between the real observations and Operator 1 data, 277.56 mm³, and the standard deviation (s), 338.39 mm³, are small compared with the values of volume observed (which range up to 220332.75 mm³). The agreements limits are -399.22 mm³ and 954.34 mm³. As shown in Figure 4, there is an agreement with a discrepancy only up to 691.31 mm³.

The Correlation Coefficient between the real measurement and that of Operator 1 ($r = 1$) confirms a direct relationship between variables.

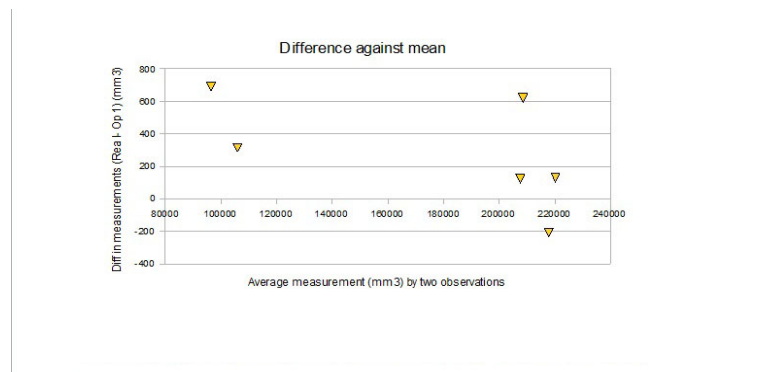


Figure 4: plot of the difference against the mean between the target measurements and the measurements of Operator 1.

The mean difference (d) between the real observations and Operator 2 data, $-193,38 \text{ mm}^3$, and the standard deviation (s), 344.67 mm^3 , are small compared with the values of volume observed (which range up to 220332.75 mm^3). The agreements limits are -495.21 mm^3 and 882.72 mm^3 . As shown in Figure 5, there is an agreement with discrepancies only up to 678.5 mm^3 . The Correlation Coefficient between the real measurement and that of Operator 2 ($r = 1$) confirms a direct relationship between variables.

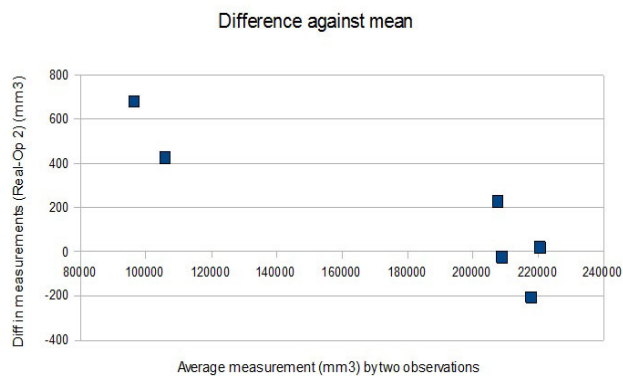


Figure 5: plot of the difference against the mean between the target measurements and the measurements of Operator 2.

The mean difference (d) between the real observations and Operator 3 data, 163.81 mm^3 and standard deviation (s), 261.51 mm^3 , are relatively small compared with the values of volumes observed (which range up to 220332.75 mm^3). The agreements limits are -359.21 mm^3 and 686.83

mm³. As shown in Figure 6, there is agreement with discrepancies only up to 586.75 mm³.

The Correlation Coefficient between the real measurement and that of Operator 3 ($r = 1$) confirm that a direct relationship between variables.

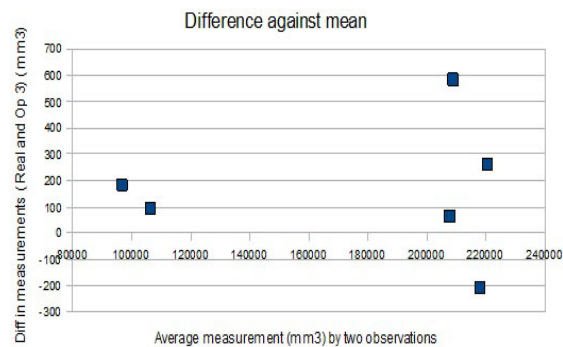


Figure 6: plot of the difference against the mean between the target measurements and the measurements of Operator 3.

The mean difference (d) between the real observations and the Operator 4 data, 108.04 mm³ and the standard deviation (s), 224.44 mm³, are small compared with the values of volume observed (which range up to 220332.75 mm³). The agreements limits are -340.84 mm³ and 552.92 mm³. As shown in Figure 7, there is a discrete agreement with discrepancies only up to 474 mm³.

The Correlation Coefficient between the real measurement and that of Operator 4 ($r = 1$) confirm a direct relationship between variables.

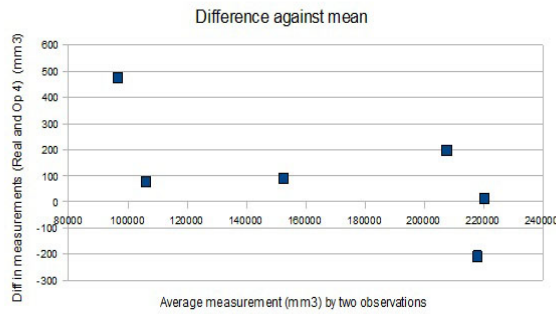


Figure 7: plot of the difference against the mean between the target measurements and the measurements of Operator 4.

The KS and T tests show that the differences between the two sets of measurements are not statistically significant. According to the KS test, the two sets of measures follow the same distribution. According to the Shapiro-Wilk test the two sets of measurements can be considered as normally distributed. According to the F test, the hypothesis of equal variance in the two sets of measurements is accepted, so in the following T-Test the Welch approximation to the degrees of freedom is not necessary. According to the T-Test on paired samples, the null hypothesis that the two sets of measures have the same mean is accepted (Table 2).

ERROR OF THE METHOD	SW	KS	F test	T test
VOLUME I	W= 0,9594 p value= 0,2188	D= 0,0857 p value= 0,997	F= 1,0385 p value= 0,9129	T= -0,2709 p value=0,7881
VOLUME II	W= 0,9608 p value= 0,2418			

Table 2. Difference test on two sets of measures of sinus volumes: SW Shapiro-Wilk test on normality; (KS) Kolmogorov-Smirnov test; (F test) F test to compare two variances; (T test) T test on equal means.

Comparing right and left sinus volumes for each Skeletal Class, no statistical differences were observed, with $P = 0.3$ (First Class), $P = 0.7$ (Second Class), and $P = 0.8$ (Third Class). Comparing all sinuses' volumes without any subdivision for Skeletal Class, no statistical difference was observed ($P = 0.2$). Similarly, no statistical difference was observed when right and left sinus volumes were taken into account. (Table 3)

Comparing the volumes of all male and female subjects, without any subdivision for Skeletal Class, no statistical difference was observed ($P = 0.1$).

	I Class <i>Right vs Left</i>	II Class <i>Right vs Left</i>	III Class <i>Right vs Left</i>
T test p=0,05	0,3	0,7	0,8
	I-II-III Class	I-II-III Class Right	I-II-III Class Left
ANOVA p=0,05	0,2	0,3	0,1

Table 3. T-test between right and left sinuses volumes (mm³) for each Skeletal Class; ANOVA results for maxillary sinuses without any subdivision for skeletal Class.

4. Discussion

In the present study, the validations of the method disclose very small uncertainties of automatic virtual volumetric analysis on CBCT scans of maxillary sinus-like phantoms. These results are supplemented by the agreement plot, where readings for the four target volumes shows a strength association between real measurement and that of each operator. Comparisons of previous validation studies show considerable variability on the experimental uncertainty; this may be due to different CBCT data acquisition techniques, segmentation procedures and choice of objects of investigation. Assessing irregular phantoms, both Uchida et al. [18] and Roth et al. [19] calculated that the mean difference was 5% or less by means of standard reconstruction based on axial slides. Posnick et al. [20] compared intracranial volume measurements on dry skulls with CT-derived measures, finding an average difference of 3.7%, while Dasti-Dar et al. reported that the relative error was within 1%, obtaining the geometrically simple volume of fluid filled syringes [21]. One reason for the more expedient results in this study may be due to manual segmentation method selecting appropriate Hounsfield unit thresholds to automatically exclude

debarred structures (i.e. impression material or bone and teeth) from the volume rendering. Another reason could be that CBCT avoids gaps between successive slices and hence provides a real 3D data-set [22].

Concerning this, the first stage of the current study assessed repeatability and accuracy of 3D measurements delivered by Dolphin software.

The RM ANOVA results (Table 1) demonstrate the repeatability of the measurements for each operator, confirming that the variability of the measurements between the various observations is not statistically significant. In addition, no statistically significant difference was observed between the data of four operators, confirming the reliability of the measurement method, independently of the observer (Table 1).

The correlation coefficient (r) showed a strong association between the real and observed measurements of each operator ($r = 1$), demonstrating the reliability of the software to identify and measure the volume of different phantoms.

For the second part of the study, the reliability of the operator who performed the measurements was tested, assessing the correlation between two different measurements performed at an interval of 30 days. The

statistical analysis showed the existence of a strong correlation between the first and second set of measurements.

Regarding the correlation between the volumes of 104 maxillary sinus and the three skeletal classes, the T test (Table 3) indicated a lack of correlation between right and left maxillary sinus size, in each skeletal class, taken individually. The ANOVA test (Table 3) shows:

1. The absence of a default size of the maxillary sinuses, in different skeletal classes, and inside each of them, and
2. The absence of correlation between the volumetric dimensions of the paranasal maxillary spaces and the three different skeletal types.

The “Sinus/Airway” volume measurement tool was then proved to be a valid and reliable instrument in the measurement of the upper airway. The setting of the sensitivity (slice airway sensitivity), the identification and design of boundaries of the sample examined (clipping boundary) are fundamental to allow a reliable measurement (with a relative error < 0.4%).

According to Alves et al, there is no established protocol for the threshold that should be used when airway volume is measured with Dolphin 3D software [16]. Although manual thresholding is more time consuming and

might generate errors if not correctly applied, it has been shown to be more reproducible when compared with the automatic technique. Indeed, El and Palomo, making a comparison between three automatic procedures and a manual segmentation technique, stated that the latter was the method with the greatest accuracy and allows the greatest operator control [23]. In attempting to establish a standardized method for using the maxillary sinus, our results show no difference in maxillary sinus volumes between male and female subjects. These data reject the hypothesis that maxillary sinus morphology is crucial to determine gender. Conversely, Uthman et Al concluded that reconstructed CT images can be used for sexing [9]. Amin et Al detected in a CT study that size of the left maxillary sinus are a useful feature in gender determination although only related to Egyptians population [24]. These previous studies focused upon taking linear measurements of the sinus using a 2D analysis, but were considered suitable for 3D characterization. The reproducibility of linear measurements is questionable when a convex shape is chosen to point out a landmark used for measurements. On the contrary, volumetric analysis of maxillary sinuses is independent from bias regarding point identification.

Our study is conducted using CBCT datasets. Currently, the technical features of CBCT scans as well as the reduced cost compared with CT scans increased their use in hospitals and dentistry. This will enhance the availability of CBCT scans in cases requiring personal identification. The independence of maxillary sinuses sizes between male and female subjects has been elucidated by the current study, which seems to refute the possibility of performing gender identification using maxillary sinuses as suggested in previous research.

Besides, taking into account different sagittal skeletal patterns as Angle's classification the independence between maxillary sinus dimensions is unchanged. This shows how the maxilla and jaw positions are independent with respect to the maxillary sinus size.

The good results achieved with this time-consuming measurement procedure support its applicability for clinical evaluation of even small changes of the antral volume in the follow-up of sinus augmentation or tooth extraction. It would be a credible goal to fully automatize sinus volume calculation and provide high accuracy at the same time.

In conclusion, the method described here has the advantage of small experimental uncertainties if it is carried out by experienced examiners. It

can strongly be recommended as a clinical diagnostic tool to gain reliable data on maxillary sinus volumes in situations where the bony boundaries of the maxillary sinuses are intact.

Conclusions

The advent of CBCT has provided the opportunity to assess the cross-sectional area and volumetric depiction of the maxillary sinus precisely with an accessible, rapid, non-invasive, and low-radiation scan. The ability to perform 3D measurements appears to be much more accurate compared with linear measurements, and reduces bias on intra-observer reproducibility due to higher accuracy of the image investigated. In previous study, important obstacles were: the influence of operator, the segmentation procedure, and 3D CBCT definition of the anatomical boundaries of the maxillary sinus.

This investigation demonstrated that, under defined clinical settings, CBCT imaging could provide accurate and reliable representations of maxillary sinus dimensions.

In conclusion:

- This validation studies, to define the experimental uncertainty, is decisive in the estimation of volumetric analysis techniques
- Confirming the availability and the reproducibility of dolphin software
- The absence of correlation between the volumetric dimensions of the paranasal maxillary spaces and the three different skeletal types
- The independence of maxillary sinuses sizes between male and female subjects

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