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Evaluation of the Reliability of an Ergonomic Decision System

by
Derek Ian Dawson

**A Thesis
Submitted to the Faculty of Graduate Studies and Research
through Industrial and Manufacturing Systems Engineering
in Partial Fulfillment of the Requirements of
the Degree of Master of Applied Science at the
University of Windsor**

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ABSTRACT

A novel approach deemed the Ergonomic Decision System (EDS) was designed to address the physical requirements of modern industry. The EDS, as the name implies, is a system that uses a series of questions and resulting choices to determine the path to the most appropriate ergonomic analysis tool for a given occupational task.

The face validity of the EDS has been established through an extensive review of literature. Reliability was evaluated both within and between subjects. In two facilities, 6 Jobs were chosen based upon both injury and illness data and the differing physical requirements of each. These Jobs were video recorded and two Jobs were randomly chosen. Novice subjects (N = 6) were asked to apply the EDS to one of these jobs prior to being provided the basic ergonomic training. Subsequently, all trained subjects (N = 12) applied the EDS to the same 6 recorded Jobs. The results from the EDS applications were then compared to a criterion measure resulting in a total EDS score which was used to determine subject *accuracy*.

A high overall mean accuracy value of 88.4%, was found with experts and novices varying only slightly with mean scores of 92.6% and 84.3%, respectively. Further, a consensus count was taken from each user for each condition to determine *consistency*. A good overall mean consensus, between subjects, of 76.9% was found with experts scoring 85% and novice subjects 72%. Also, the results of the pre-post training study indicated strong within subject consensus with an average of 88.9% across novice subjects. Finally, after a minimum of two weeks had passed, all subjects applied the EDS to the second randomly chosen Job. Results of the test-retest condition showed good consensus within subjects with a mean of 94.4%, where experts scored 88.9%, and novice subjects showed perfect consensus. The results of the study effectively establish that the EDS provided sufficient subject *consistency* and *accuracy* in directing subjects to the most applicable ergonomic resource across Jobs tested.

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... this is what you know ... this is what I know ... this is where we both know nothing ~
Anonymous

I would like to thank my family for their support and reassurance. Dad, your methods aren't always conventional, yet who can argue with results. Tracy, you are an angel. Aunt Bonnie, Uncle Dan, Uncle George, Aunt Faith, throughout my life you helped me to see the bigger picture.

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This Thesis is dedicated to my mother, the late **Sandra L. Dawson**. She is missed constantly.

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Chapter I

INTRODUCTION

Despite advances in work mechanization and the implementation of positioners and handling devices, manual materials handling (MMH) is still very common within the contemporary industrial environment (Aghazadeh, 1998). Rationales favouring direct human interaction with the component or media are many. Some of the most prevalent include: space limitations, the varied nature of the activity which necessitates human cognition and three-dimensional perception, and the reluctance to make substantial investment in manual manipulation devices, automation or hybrid semi-automation (Mital, Nicholson & Ayoub, 1993; Akella & Peacock, 1999).

Physical work entails the application of some physical energy (effort) against opposing forces within the immediate physical environment. The application of force is generally not of concern but rather it is the resistance, both internal and external, that elicit a response from the body (Zetterberg & Ofverholm, 1999). This may be better defined by Newton's second law, which stipulates that, for every applied force, there is necessarily an equal and opposing force (Elliott & Wood, 1995). Physical work required in modern industry places many and varied physical demands on the worker. It is the sum of the applied efforts that challenge the worker's musculoskeletal system. The response of these systems to the demands of a task are bounded by the biological laws of the body, that is to say that there is an inverse relationship between tissue tolerance and physical demands (Mital et al., 1993).

Historically, the main focus, of preventative measures to avoid physical overexposure, had been on manual lifting (NIOSH, 1981). There are, however, a greater variety of MMH conditions to which employees within automotive manufacturing facilities may be repeatedly exposed including: pushing, pulling, lifting, lowering, carrying, and hand-intensive work (Sanders & McCormick, 1993). Further, while performing these tasks, work requirements may necessitate the use of one or two hands or body parts, statically or dynamically over a number of

frequencies in anatomically neutral, deviated or awkward postures. Predictably, with each novel combination of posture, action and frequency, a unique set of physical challenges is imposed upon the worker. In order to preempt physical strain, each novel situation then requires a unique analysis process.

The United States reports annually on the occurrence of injuries and illness and provides a categorical breakdown of these within private industry. The data is compiled through an annual survey conducted by the United States Department of Labor, Bureau of Labor Statistics (BLS). This data can be used as an indicator of injury and illness trends through industry, body component, traumatogens and a host of other metrics (NIOSH, 1997; Rosecrance & Cook, 1998). Recent data shows that although total incidence of injuries and illnesses are declining, work related musculoskeletal disorders (MSDs) attributable to MMH are on the rise (BLS, 2003). Within private industry, more than a third of occupational injuries and illness' are attributable to overexertion and repetitive motion (Sanders & McCormick, 1993; Konz, 1995; GAO/HEHS, 1997; NIOSH, 1997; OSHA, Federal Register, 1999; IE, 2003). Of particular interest, recent data indicates that the category of overexertion, defined as injuries resulting from excessive lifting, pushing, pulling, carrying, or throwing objects, grew significantly (IE, 2003). This category now alone constitutes more than twenty five percent of all injuries (IE, 2003).

Costs associated with MMH represent approximately 60% of all monies spent on industrial injuries (Konz, 1995; GAO/HEHS, 1997)). Direct costs of manual handling injuries and illnesses are estimated to be between 13 billion and 20 billion dollars annually (Mital et al., 1993; NIOSH, 1997; IE, 2003). While direct costs are significant, it is only a portion of the total costs. Indirect costs, including overtime, training, lost productivity and other contributors are estimated to amount to between three and five times direct costs (Mital et al., 1993; IE, 2003).

Within the private sector, the automotive manufacturing industry has consistently been implicated as being among the top contributors for incidence rates and sheer numbers of injury and illness cases (NIOSH, 1997; BLS, 2003). The enormous volume of workers annually

employed by the auto industry tends to amplify the necessity for intervention. For example, in 2001 the BLS category of motor vehicles and car bodies (SIC 3711) was second on the list of private sector industries with the highest incidence rates for injuries and illnesses attributed to repetitive motion (BLS, 2003). The enormity of its population, however, produced an exorbitant number of cases (22,900) that were approximately twice the case rate of the industry topping the list.

As with any materials, the elements that make up the musculoskeletal system have tissue tolerance thresholds beyond which failure (in the case of humans, injury or illness) occurs (Snook, 1978). There are a number of variables which contribute to the potential for tissue failure, some of these include; the magnitude of stresses placed upon the body segment, the frequency with which stresses occur and the interval between stressors (Winkel & Westgaard, 1992; Kilbom, 1994). Tissue failure may be either acute or chronic. Acute traumas are a result of a single load exceeding the tolerance of the tissue. In the case of chronic injuries or illnesses, failure occurs from repeated loading over a long period of time (Putz-Anderson, 1988b).

In an industrial setting, injuries or illnesses are known by a number of terms. Some of these are defined by the body segment or joint within which they occur, such as occupational cervicalbrachial disorders (OCD) for the shoulder region, upper extremity cumulative trauma disorders (UECTD) and low back pain (LBP). Other terms are more generic such as, repetitive strain injuries (RSI), cumulative trauma disorders (CTD), musculoskeletal disorders (MSD) (Rosecrance & Cook, 1998). The repetitive and forceful movements, and postures characteristic of manual materials handling within the automotive industry, have been implicated as individually causal and multiplicative risk factors associated with many of the disorders previously mentioned (Kvarnstrom, 1983; World Health Organization [WHO], 1989; Marras & Schoenmarklin, 1993; Baron, 1996;). Within the automotive manufacturing sector there are many operations which require one or more physical stressors including; high levels of force, high rates of repetition and awkward or sustained postures. These physical stressors have been

shown to be risk factors for the development of acute or cumulative injury or illness (NIOSH, 1977; Putz-Anderson, 1988a; Putz-Anderson, 1988b; Kroemer, 1989; Moore et al., 1991). Further, these stressors may concur and interact serving to amplify the risk of injury or illness (Silverstein et al. 1987; Kilbom, 1994b).

There are a variety of approaches which may be used in order to assess MMH capabilities over a number of working conditions. These intervention techniques include epidemiological studies, the identification of biomechanical and physiological limitations and psychophysics (Mital, 1993; Sanders & McCormick, 1993; Konz, 1995;). Each approach has functional constraints. These constraints are limitations bounding the assessment methodology which, if acknowledged, will ensure that the most appropriate approach will be used for each occupational analysis.

Epidemiological studies examine the relationship between work and morbidity patterns in human populations (Friedman, 1974). This approach requires a lot of time and resources to collect this type of data (Hennekens & Buring, 1987). It further assumes that historical health data exists, is accessible and is accurate.

Biomechanical methodologies view the human body as a system of segments interconnected at joints. Knowledge of the properties of each segment need to be attained as well as corresponding joint type. From this a model may be developed with each segment and link representing the same properties as the corresponding human segments. Biomechanical criteria are frequency independent, meaning that a tissue safety threshold, as established through research, is applicable only to very low frequency manual materials handling. As frequency increases efforts should decrease, therefore as frequency increases a more appropriate evaluation tool is required. Biomechanical models are not designed to address repetitive work and fatigue issues (Mital et al., 1993).

Physiological research provides detailed physical responses to a variety of occupational conditions to which a worker may be commonly subjected. This type of research measures heart

rate, oxygen consumption and energy expenditure. The data has been used to develop physiological thresholds at which the risk of injury or illness increases. Studies of fatiguing conditions have been used to propose work-rest ratios for a variety of work parameters (Rohmert, 1973; Rose et al., 1992). Physiological methodologies have been found to be most applicable to high frequency work and work over extended durations (Andrews, 1967; Garg & Saxena, 1982). The psychophysical approach to analyzing MMH conditions records the worker's perception of physical stress, exertion and fatigue or discomfort while completing a task (Snook, 1978; Legg & Myles, 1981; Foreman et al., 1984; Ljunggren, 1986; Fernandez et al. 1991;). The premise is that a worker will combine both biomechanical and physiological stresses in their subjective evaluation of perceived stress (Gamberale et al., 1987; Sanders & McCormick, 1993; Gescheider, 1997). Further, symptoms associated with working conditions as mentioned previously, are thought to be early indicators of work-related injuries or illness' (Yoshitake, 1971; Karwowski & Yates, 1986; Baidya & Stevenson, 1988).

There are many ergonomic tools, aids and guidelines in existence, each of which makes use of one or all of the analytical methodologies discussed above in order to assess working conditions. Some are body segment specific, such as those designed to evaluate work of the upper extremity (McAtamney & Corlett, 1993; Keyserling et al., 1993; Fisher et al., 1993; Kilbom, 1994; Rosecrance & Cook, 1998; Bergamasco et al., 1998; Muggleton et al., 1999), shoulder (Dul, 1988; Winkel & Westgaard, 1992) and back (Frymoyer et al., 1980; Marras et al., 1995). Other assessment methods analyze the entire body through a variety of postures, forces and frequencies (Rodgers, S.H., 1992; OSHA, 1995) and yet, others tend to focus on specific job elements (which imply physical actions) such as pushing, pulling, carrying, lifting, lowering and hand intensive work (Snook and Ciriello, 1991; Mital et al., 1993; Waters et al., 1993; Snook et al., 1995; Snook et al., 1997; ACGIH, 2000). There exist alternative analytical devices that may be used to supplement some of the aforementioned ergonomic prevention strategies. These consist of intricate equipment and techniques in order to quantify the effort requirements of a task

or series of task elements. Some methods include electromyography, often in conjunction with cinematography, the use of accelerometers, electrogoniometers and force dynamometers. Each of these analytical methods varies in: 1) the level of complexity required to use it, 2) the required invasiveness during collection and 3) the tool's ultimate sensitivity and specificity. Each has its application limitations and many are redundant. Modern industry requires an ergonomic analysis process containing a tool set that closely correlates with some form of outcomes measures (symptoms data or injury, illness data). Further, the process must be: 1) able to be used by the majority of individuals with the proper training, 2) timely and relatively non-invasive, 3) reliable across and between users, and 4) the risk assessment tools included must show a good balance between sensitivity and specificity.

If the analysis process exhibits poor sensitivity, an unacceptable level of false positives will result. This, in turn, becomes very costly to the company in a number of ways. Firstly, the ergonomics system will become overburdened by requiring the in-depth analysis of operations that do not require intervention (Joseph et al., 2000). Second, the result would be an unnecessary, large financial impact to companies that can employ as many as hundreds of thousands of workers. It is, therefore, necessary that the analytical methodology adopted by an ergonomics program be critically reviewed and evaluated for both its validity and reliability.

The Ergonomic Decision System (EDS) was designed to address the variety of occupational conditions, to which employees within automotive manufacturing facilities may be repeatedly exposed with the direction to preempt ergonomically unsound conditions. In order to do this, the developers of the EDS needed to identify common physical actions required for MMH within the workplace. Further, it needed to be established whether there were means to review these actions for ergonomic suitability. What was essentially required was a gaps analysis, making use of the constraints and limitations of adopted ergonomic intervention tools and seeking-out methods to resolve these. The Ergonomic Decision System as the name implies, is a system that uses a series of questions and resulting choices to determine the path to the most

appropriate ergonomic analysis tool for a given occupational task. It is hypothesized that the EDS will be useable by virtually any trained individual. Further, the system is intended to ensure consistent and reproducible analyses.

The structure and content of the EDS were developed over an exhaustive series of technical meetings with experts in the field of automotive ergonomics. The ergonomic tools embedded within the EDS feature the most recent, critically reviewed and agreed-upon scientifically based ergonomic knowledge to date. The development of the EDS represents an attempt at formalizing efforts to evaluate ergonomic risk proactively and consistently within an automotive manufacturing Company. Though other studies have attempted to preempt ergonomic risk by way of checklists and various techniques (Rodgers, 1992; Keyserling et al., 1992; McAtamney and Corlett, 1993; OSHA, 1995), many were proven to exhibit poor sensitivity and lack consistency in results (Keyserling et al., 1992; Joseph et al., 2000).

Prior to the advent of the Ergonomic Decision System (EDS) there did not exist a formalized ergonomic decision process which met automotive manufacturing industry requirements. In order to meet sensitivity and specificity criteria, it was necessary that each ergonomic tool, used within the EDS, be adopted based on consensus scientific evidence, expert opinion and operational application. It is essential that the EDS content validity be proven, in order to ensure sufficient sensitivity and specificity (Joseph et al., 2000). This will be accomplished via an in depth literature review. In order for the EDS to be useful, it must be able to be repeatedly and accurately applied by multiple analysts. Reliability of the EDS will be established by having trained experts and novices independently use the EDS on the same operations under the same time constraints.

1.1 Statement of Purpose

The purpose of this thesis is to establish the reliability and face validity of a unique ergonomic process, deemed the Ergonomic Decision System. Though based on universally applicable research, the EDS was designed to be used within the automotive manufacturing sector.

Face validity will be established via an in-depth literature review, from which the content of the decision system was developed. The between and within-rater reliability of the decision system will be established from controlled testing with a number of trained ergonomic engineers and novices working in isolation, under time restrictions and using the process in an attempt to analyze several jobs. Particularly this study seeks to determine if the EDS is reliable across individuals (both expert and novice) and meets established time requirements such that it can be shown to be a relatively non-invasive and comprehensive tool.

1.2 Statement of Hypothesis

It is hypothesized that both expert and novice subjects, trained on the ergonomic decision system, will reliably arrive at the same decision with regard to the appropriate ergonomic tool while observing the same operation under the same constraints.

Chapter II

REVIEW OF LITERATURE

A substantial body of evidence exists to support the implementation of an ergonomics process within the industrial manufacturing sector (OSHA, 1999). The evidence is based on two premises; first, that there is a positive relationship between work-related musculoskeletal disorders and workplace risk factors and second that an effective ergonomics process can reduce the potential for these injuries and illnesses (NIOSH, 1997; NAS, 1998).

One may ask why a company would expend resources on such an endeavor? It is expected that within society today a corporation has an obligation to its employees, their families and the community at-large to act in a manner which does no harm (Department of Labor & Industries, 1988; WCB, 1994). In many unionized environments this is contractually enforced. An ergonomic convention is typically found within these contracts (UAW-Ford Motor Company, 1999). Further, within the United States, an attempt to legislate ergonomics as a component of industrial processes was recently brought forth (OSHA, 1995; OSHA, 1999). Finally, there are financial benefits inherent to the institutionalization of an ergonomics program. Some of these include the provision of a larger pool of workers capable of completing work tasks, the prospect of reduced workers compensation claims, decreased absenteeism, increased productivity and increased quality (Eastman Kodak Company, 1986). The astute corporation adopts ergonomics, for a number of the above reasons. It seems implicit that the benefits of the implementation of a sound ergonomics process far outweigh the costs (Oxenburgh, 1991; Barsky & Dutta, 1997; Busse & Bridger, 1997; GAO, 1997; Burrows et al., 1998).

The Ergonomic Decision System (EDS) serves as an integral component of the ergonomic process within a large automotive manufacturer. It is designed to preempt musculoskeletal disorders by having the user break an entire job into its component elements. Subsequently, approved ergonomic analysis tool offerings are used to scrutinize each element as the user is asked a series of prompting questions. Each question serves to progressively filter the

input data until only the pertinent information remains. The remaining data is then run-through the most applicable ergonomic tool. The output is a passing or failing condition for each work element. The EDS is intended to be used proactively, in the early stages of the design process but may be used reactively as necessary. It is postulated that a review of the research composing the EDS will serve to provide evidence of content validity.

Human capacities are determined by work elements such as force, posture and repetition. Each of these elements has been individually and collectively studied in an attempt to quantify the relationships between imposed physical stress and the resulting strain. The research approaches used include biomechanics, physiology, psychophysics and epidemiology. Each approach is unique and will be discussed individually. The culmination of approaches will serve as the research basis of the EDS.

2.1 Ergonomic Analysis Techniques

2.1.1 Biomechanical

As the name implies, biomechanics is the study of energy and forces and their effect on biological systems (Merriam-Webster's, 1993). Research in occupational biomechanics utilizes the laws of physics to estimate the stresses imposed upon the musculoskeletal system under working conditions such as the actions required during the manual handling of materials. The biomechanical approach treats the human body as an intricate system of soft and osseous tissues acting as pulleys and levers. The levers (body segments such as lower leg or forearm) are empowered to move because of a strategically balanced mass-spring-damper composite. Osseous tissue or bone and joints act as rigid bodies and are essentially the systems foundation. Soft tissues, particularly muscles and tendons serve all three roles within this system; as a component of the levers mass to be moved, as pulleys or springs with potential energy waiting to be converted to kinetic energy by way of concentric contraction and as dampers, ensuring stability with eccentric contractions (Eastman Kodak Co., 1986; Tracy, 1990; Sanders & McCormick, 1993).

Forces acting on the system either externally (mechanical force on external surface) deemed exposure, or internally (pressure and mechanical force of soft tissues on bones or ligaments) deemed dose, elicit a response. The bodily response depends on a number of potential traumatogens which serve to amplify the effects of the initially applied force (Kilbom, 1994b). The fundamental contributor is the amplitude of force required and the conditions under which the force is applied (Eastman Kodak Co., 1986). Potentially harmful occupational conditions include time alterations in both the application of force and segment postures. These two time-weighted factors are collectively known as repetition (Kroemer, 1989). Further, the severity of the posture itself tends to lengthen or shorten the active muscle. The length of a muscle is important to its ability to produce tension. When a muscle changes in length from its resting state, contraction efficiency decreases. The overall resulting force of a contracting muscle (total tension) therefore also decreases (Chaffin et al., 1999). As with any materials, the elements which make up the human kinetic segments have tissue tolerance thresholds beyond which failure (in the case of humans, injury or illness) occurs (Snook, 1978).

Various biomechanical models have been produced in an attempt to predict and provide guidelines to control for physical overexertion. Most of these exist within published literature and some are available as proprietary devices and software (Park, 1973; Armstrong et al., 1979; Greene & Wolf, 1989; Radwin et al., 1991; Loslever & Ranaivosoa, 1993;). Researchers at the University of Michigan, Center for Ergonomics, developed a model designed to analyse population or individual physical capabilities given various operational inputs (Keyserling & Chaffin, 1986). These two and three-dimensional models were then developed into proprietary software for distribution. The output of the models include percentage of the population capable of exerting the required effort by joint, and an estimation of the compressive forces on the lower back. Biomechanical modeling can aid the analyst in the evaluation of many aspects of manual materials handling, whether completed by the individual and compared against physical

thresholds established through experimental research or by entering values as required into a pre-existing analytical model.

2.1.2 Physiological

The physiological analysis technique addresses the biological limitations of the human during long duration, repeated physical exertions where the load applied is within the physical strength of the worker. It is unlike the biomechanical approach, which is generally used to analyze low frequency physical efforts (Mital et al., 1993). The manual handling of materials within an industrial manufacturing environment often requires the rapid and repeated application of effort. During this type of work the force requirements are not usually the limiting factor, but rather it is muscular fatigue that limits the workers endurance (Snook & Irvine, 1969; Hagberg, 1981). During high intensity work, the muscles of the body must work more efficiently. To do so, they require a higher volume of blood flow, carrying oxygen and nutrients to the working tissue and sweeping away waste byproducts such as lactic acid. If the demand for these essential system elements exceeds the supply, the activity will not be able to be continued (Andrews, 1967; Astrand & Rodahl, 1986; Eastman Kodak, 1986).

With knowledge of the physical responses to tasks requiring some level of endurance, physiological methodologies can focus on the measurement of heart rate, measures of oxygen consumption, and further energy expenditure criteria in order to describe and establish physical thresholds (Garg & Saxena, 1982; Garg, 1983). Metabolic energy expenditure is among the most widely measured and accepted physiological response to repetitive materials handling as it is directly proportional to the workload at steady-state conditions (Mital et al., 1993). As such, the proportion of metabolic expenditure required may be compared to a criterion measurement for work under a given set of physically taxing conditions (Garg et al., 1978). Several equations have been developed for predicting energy costs for a number of manual handling scenarios (Rohmert, 1973; Genaidy & Asfour, 1987; Rose et al. 1992). Each of these account for certain variables as body weight, weight of load, gender, vertical start and end height of lift, dimensions

of the load, frequency and duration of work (Sanders & McCormick, 1993). The ergonomic threshold for working is impacted by these qualifiers.

2.1.3 Psychophysical

When biomechanical or physiological data are unknown, difficult to apply or impractical techniques to be used, psychophysics serves as a method of evaluating a variety of working tasks. This alternative approach entails subjects adjusting either effort (load) requirements or exertion frequency (load held constant) while performing a task to the maximum amount that could perceptually be sustained for some prescribed period of time (Snook & Ciriello, 1991; Mital et al., 1993). Periodically ratings of perceived exertion, physical stress or fatigue are measured (Borg, 1973). The theory is that since fatigue has been identified as an early symptom of use-related musculoskeletal disorders (MSD), the psychophysical method may serve as a sensitive indicator of MSD risk (Hagberg, 1981; Borg, 1982; Habes et al., 1985; Basmajian & Deluca, 1985; Baidya & Stevenson, 1988; Potvin & Bent, 1997).

One of the benefits of psychophysics is that it allows the interacting effects of differing physical stressors be evaluated at the same time. The ratings obtained through this method are the result of the central nervous system attempting to understand peripheral sensations and physiological state. All of the inputs are integrated, referenced against experience and memory and output as psychophysical ratings (Gescheider, 1997). Psychophysical methodologies have been used extensively in the design and evaluation of a variety of manual materials handling tasks (Snook & Irvine, 1968; Legg & Myles, 1981; Garg & Saxena, 1982; Ciriello et al., 1990; Snook et al., 1995; Snook et al., 1997). The 1991 NIOSH committee used the psychophysical criterion in the development of its equation designed to protect workers throughout a variety of lifting durations and frequencies. The committee decided to establish a lifting effort threshold which would be acceptable to 75 percent of the female working population. Further, this value was proposed to ensure acceptability to veritably all male workers. The rationale for the use of the 25th percentile female population strength value, was based on the findings of Snook (1978). He

based his findings on insurance data and stipulated that a worker is three times more susceptible to low back injury if performing a manual task that is acceptable to less than 75% of the working population. The psychophysical methodology has been proven to be a quick, consistent and reproducible means of assessing physical limitations during typical manual material handling tasks (Wardle & Gloss, 1978; Krawczyk et al., 1993). Several studies have reported that psychophysical studies need not take place over a representative 8-hour work day, or even a typical 5-day work week (Legg & Myles, 1981; Legg & Myles, 1985; Ciriello et al., 1990). In fact, several studies indicate that a subject is able to accurately determine an acceptable load or frequency, for a variety of manual handling tasks, within two hours of testing (Snook & Irvine, 1968; Snook, 1978; Ljungberg et al., 1982; Fernandez et al., 1991; Snook et al., 1997; Snook et al., 1997). Karwowski and Yates (1986) found that at lifting frequencies of six per minute or less, subjects could choose acceptable weights within 30 minutes that did not differ significantly from those chosen after four hours work.

Mital (1983) however, did not find that subjects could estimate an acceptable, perceived load while working for 20 – 30 minutes. It was stated that individuals taking part in a psychophysical lifting study would tend to overestimate their respective maximum acceptable weight of lift. These findings may be due in part to experimental design. It was found that individuals would tend to choose higher workloads while adjusting the frequency with a constant load rather than load with a constant frequency (Nicholson & Legg, 1986). Further, at higher working frequencies the psychophysical method may overestimate physiological capabilities (Ciriello & Snook, 1983; Karwowski & Yates; 1986). In a study conducted by Mital (1985), psychophysical and physiological data were collected simultaneously. Findings indicated that for manual lifting at a frequency at or below 4 actions per minute the psychophysical criteria should be considered more reliable (Mital et al., 1993). Karwowski and Yates (1986) stipulate that the psychophysical methodology should not be used to assess lifting capacity at a frequency above 6

lifts per minute. From this we may establish that the upper frequency threshold for the use of the psychophysical methodology is between 4 and 6 actions per minute.

2.1.4 Epidemiological

Epidemiology is the study of how often diseases occur in different groups of people and why these occur.(Coggon, Rose & Barker, 1997). Translated into an occupational sense, the emphasis of epidemiological research is on the measurement of injury or illness outcomes within a working environment, as they relate to a population at risk (Sommerich et al., 1993). Essentially, epidemiological studies seek to establish a relationship between workplace exposure and physical effects. Measurements of risk include; counts (number of people within a group suffering from some prescribed injury or illness), prevalence rate (number of people in a group suffering from some injury or illness/total number of people within the group) and incidence rate (number of people developing a disorder/total number at risk)/unit time). These measurements can then be used to compare occurrence of the prescribed disorder among different groups (Mital et al., 1993). From these comparisons, occupational risk factors of manual materials handling (i.e. load characteristics, posture, repetition rate, duration) may be identified (Andersson, 1981). Once identified, an attempt may be made to establish the strength of the relationships between risk factors (Chaffin & Park, 1973; Silverstein et al., 1987).

The relative contribution of each risk factor (force, posture, repetition etc.) has been the focus of many studies (Kadefors et al., 1976, Silverstein et al., 1987, Keyserling et al., 1993, Hagg et al., 1995, Engstrom et al., 1998). It is generally assumed that force is the key contributor to disorders, and deviated posture tends to amplify these forces, whereas, repetition alone depicts the temporal relationship between deviations in posture and also the application of force, as required by the cyclical work (Silverstein, 1985; ACGIH, 2001). Several studies have sought to establish an exposure-response relationship between different body areas, forceful and repetitive work (Herrin et al., 1986; Schoenmarklin & Marras, 1993; Loslever & Ranaivosoa, 1993;

Schoenmarklin et al., 1994). The results of these may be used to identify workplace risk factors and can provide 'benchmarks' to identify and preempt occupational risk factors (Lee et al. 1997).

Based on epidemiological studies, Armstrong et al. (1982, 1996) and Silverstein, Fine, and Armstrong (1987) established repetition as a risk factor for CTDs. In two cross-sectional studies, Silverstein et al. (1986-87) reviewed 4 groupings; low force-low repetition, high force-high repetition, low force-high repetition, high force-low repetition. From these studies it was found that the risk of a CTD injury in low force-high repetition jobs was 3.3 and 2.7 times respectively greater than low repetition jobs. Stock (1991) reviewed 54 studies, and concluded that specific disorders of tendons and tendon sheaths are causally related to repetitive and forceful work. Armstrong et al. (1993) reviewed 22 studies of occupational groups, which met the criteria of intensive hand-work and/or repetitive use of the hands and wrists. Carpal tunnel syndrome and tendonitis of the hand-wrist were among the most frequently occurring musculoskeletal disorders identified. Kilbom (1994b) sought to evaluate work of the upper extremity by reviewing scientific literature with specific regard to the exposure-effect relationship. This extensive review of epidemiological studies, cited 17 that had established an dose-response relationship between repetitive and forceful work and musculoskeletal disorders. Latko et al. (1997) reviewed 13 selected epidemiological studies that show a relationship between repetitive work and upper extremity disorders. This study established that the dynamic nature of modern industrial tasks must be considered, in addition to the number of motions and the amount of idle time. The National Institute for Occupational Safety and Health (NIOSH) performed extensive research on musculoskeletal disorders in the workplace (1997). This was founded on the concept that, when occupational demands repeatedly exceed the biomechanical capacity of the worker, the activities become trauma-inducing. The study featured a critical review of epidemiologic evidence by occupational CTD and affected body part. Results indicate that there is strong evidence of a positive association between exposure to a combination of risk factors and injury or illness (NIOSH 1997).

The Occupational Safety and Health Administration (OSHA) of the U.S. Department of Labor, performed an extensive review of epidemiological, laboratory and psychophysical evidence (OSHA, 1999). The epidemiological evidence, concurs with previous findings that the risk factors of force, posture and repetition are individually implicated as risk factors for CTDs. It is noted however that the cumulative and multiplicative effect of these is of greater concern.

The epidemiological approach may produce useful insight into ergonomic risk factors and their relative contribution. These results may be adopted in the design of operations within manufacturing assembly facilities. It should be noted however that methodology used for these studies should be heavily scrutinized for experimental design and statistical significance (Mital et al., 1993). Further, the results from these studies are often qualitative due to the lack-of or difficulty obtaining, quantitative outcomes (injury/illness) data.

2.2 Ergonomic Risk Factors

Job analysis, by way of the EDS is useful for identifying sources of injury and illness before these are manifested in claims. Moreover, the EDS can be used to evaluate up-front design or improvements in job and tool redesign without having to wait until claims are actually produced or reduced. The EDS includes a method for measuring the workers exposure to each of the primary risk factors: force, posture and repetition. The exposure is then compared to known human capabilities to compute an injury probability. A risk factor is defined as an attribute or exposure that increases the probability of the disease or disorder (Putz-Anderson, 1988b).

Occupational risk factors include repetitive and sustained exertions, awkward postures, and high mechanical forces (Selan, 1994). These primary risk factors will be defined and discussed below.

2.2.1 Force

Mathematically forces represent the efforts necessary to produce or resist movement. This does not mean that every force produces a movement, in many instances acting forces are balanced so that no movement is produced. In fact, an occupational task may require the combination of static and dynamic work (Frankel & Burstein, 1970). The external effect of a force tends to

change the velocity of the body. A general principle is that a body moving at a constant velocity requires a force to change this velocity. A stationary body has zero velocity and thus requires a force to change its state. A body moving at a constant velocity however, is said to be in a state of dynamic equilibrium (Chaffin & Andersson, 1991; Elliott & Wood, 1995).

Forces developed by the muscle-tendon complex act on bones at their points of insertion and cause a rotational moment, or torque, around a joint. The muscles and bones act as a series of levers. For example, when a worker lifts a box with both arms, the box acts as a load or resistance on a lever, in this case the forearm (Rodgers, 1986). When the force requirements of a job exceed worker capacity repeatedly or with a single occurrence, overexertion injuries or illnesses can occur. The threshold limit values (effectively worker capacities) for use within the EDS have been extrapolated from epidemiological and experimental studies. The force constraint varies by both muscle group utilized, and combined risk factors. For example, as frequency increases, force application capabilities decrease (Hagberg, 1981; Garg & Saxena, 1982; Habes et al., 1985; Krom et al., 1990; Rempel et al., 1992). The acceptable force value adopted by the EDS varies according to action reviewed, direction and frequency of application, number of hands utilized, and postures assumed.

2.2.2 Posture

It is generally assumed that force is the key contributor to MSDs, and deviated posture tends to amplify these forces. That is to say, as a joint is moved out of its natural or anatomically neutral posture, there is a corresponding reduction in strength capability (Karhu et al., 1977; Snook & Ciriello, 1991). These reductions are not necessarily linear and are unique by body part (McAtamney & Corlett, 1993; Mital et al., 1993). The EDS employs the logic obtained from several research papers and existing software programs and applies these as a portion of the whole analysis for each work element reviewed.

2.2.3 Repetition

Repetition, though difficult to isolate, is implicated as an ergonomic risk factor. Although there are not yet any universally accepted guidelines, several studies, both epidemiologic and experimental have adopted definitions to suit the particular situation (Armstrong et al., 1982; Silverstein, 1985; Kilbom, 1994b; Marras et al., 1995). Repetitive movements in industrial tasks have been shown to be an important risk factor associated with cumulative trauma disorders (CTDs) (Silverstein et al., 1987; Marras & Schoenmarklin, 1993). For example, operational activities involving repetitive movements that produce muscular tension are indicated often to be associated with various occupational upper extremity disorders (Kvarnstrom 1983; Habes, Carlson & Badger, 1985; Feuerstein and Fitzgerald, 1992; Mital et al. 1993).

The EDS utilises a variety of different repetition values as a determination of which particular ergonomic tool would be most applicable in a given situation. The value used is determined by the particular action reviewed. For example, where repetition is reviewed in isolation, studies indicate that an individual is able to repeat movements much more for smaller muscle groups than larger (Kilbom, 1994b). With this understanding, lifting tasks, which tend to require large muscle groups may be deemed frequent (repetitive) at work rates of 1 or 2 lifts per minute. Conversely, hand intensive tasks, which tend to utilize several small muscle groups, may be considered repetitive at 10 or more wrist movements per minute (Kilbom, 1994b). Further, fine-finger work, such as typing, may not be viewed as highly repetitive until 200 motions a minute (Kilbom, 1994a).

2.3 Ergonomic Decision System (EDS)

The EDS methodology consists of dismantling an operation (proposed or existing) into its constituent elements. Each of these elements may then be scrutinized for specific physical requirements. Once the particular physical requirements have been established, these may be compared to the most appropriate and consensus-driven ergonomic thresholds for the given

analysis. The source of information for each of the elements and decision variables will be reviewed, highlighting the research methodology and the logic behind the choice.

The elements included within the EDS include both actions and required postures. These have been established via consensus and are deemed to constitute the most common physical manifestations within the automotive assembly environment. It was decided that rather than reviewing the thousands of individual components which make-up an automobile a holistic approach would be taken which should encompass the majority of actions and postures required during the assembly process. Initially, the user of the EDS is prompted to identify particular work tasks and subtasks required in order to complete the working task. Once these are determined, the user is prompted to choose from among four actions and three postures, each describing one work element. The four action choices are; pushing or pulling, carrying, lifting or lowering, and hand intensive tasks. The three posture variables include; static work, awkward postures and overhead work.

It was felt that by including these elements, the EDS would sufficiently address much of occupational conditions promoting injury and illness. These actions and postures are identified within United States Department of Labor, Bureau of Labor Statistics. The categories within which these elements are contained include overexertion and repetitive motion. As mentioned previously, these categories alone represent more than one third of all occupational injury and illnesses within private industry (Sanders & McCormick, 1993; Konz, 1995; NIOSH, 1997; OSHA, Federal Register, 1999; IE, 2003). It was the desire of the developers of the EDS to incorporate the most applicable and consensus driven tools, aids and guidelines into the process. These will be reviewed looking at the research methodology and a discussion of the assumptions and limitations of each.

2.3.1 Psychophysical Approach in EDS

Psychophysical studies of various manual handling tasks have been conducted by Liberty Mutual over the past three decades (Snook & Irvine, 1968; Snook & Irvine, 1969; Snook, 1978; Snook,

1985; Snook & Ciriello, 1991; Snook, Vaillancourt, Cirello, Webster, 1995; Snook, Vaillancourt, Cirello, Webster, 1997). A variety of tables constituting physically perceived thresholds were developed over this time. The work tasks performed within the Liberty Mutual studies were unique, in that they attempted to mirror industry as closely as possible. For example, the manual handling of materials was dynamic, not isometric. The tasks took place over a series of distances and frequencies, closely emulating those found in industry (Snook, 1985). Further, the studies occurred over several sessions lasting between 4.5 to 8 hours and took place over several weeks (Snook, 1978; Snook & Ciriello, 1991; Snook, 1995; Snook, 1997). It is through these carefully controlled experiments that the Liberty Mutual studies have attempted to develop guidelines for the evaluation and design of manual handling tasks that are consistent with worker capabilities and limitations (Snook & Ciriello, 1991).

The original studies published in 1978, reviewed and compiled the findings of several experiments that depicted the maximum acceptable weights and forces for the actions of lifting, lowering, pushing, pulling and carrying tasks (Snook, 1978). The methods employed with each novel action varied out of necessity. However, the primary analyses technique, psychophysics remained constant throughout. Essentially, the worker was given control of the force variable (usually the weight of the object being manipulated). All other variables such as frequency, size, height, distance etc. were controlled (Snook, 1985).

In order to overcome adaptation effects, each manual handling task was broken up into two segments; the first with a heavy initial weight, the second light. The subjects were then instructed to make adjustments to the weight until a comfortable level had been achieved. If the results of the first segment were within 15% of the second, the average of the two results was recorded, if not results were discarded (Snook, 1978). The results of all experiments were integrated into a series of tables containing maximal acceptable weight limits for these manual handling tasks. It was however noted that not all of the values contained within the table were experimentally derived. Assumptions were used to fill-in the gaps (Snook, 1985).

Four additional psychophysical studies took place designed to fill-in some of the missing components within the Liberty Mutual tables. The first experiment used 10 male and 12 female subjects to investigate the effect of frequency on maximum acceptable weights and forces (Snook, 1985). Fifty-one variations of seven tasks were reviewed (Snook & Ciriello, 1991). Tasks included, four lifting or lowering, two pushing and a carrying task. These are the same values used by Snook in previous experiments (Snook, 1978; Snook, 1985; Snook & Ciriello, 1991). The second experiment investigated the effects of object size, lifting distance and pushing or pulling height (Snook, 1985). Experimental methodologies were identical to previous experiments save the aforementioned variations and the subjects. Subjects were 12 female industrial workers. The subjects performed 61 variations of these work elements (Snook, 1985).

The third experiment investigated the effects of task duration on maximum acceptable weights and forces (Ciriello et al., 1990; Snook & Ciriello, 1991). Previous experiments used a 4-hour duration consisting of five different 40 minute tasks, with 10 minute breaks between each task. In this experiment, the same task was performed continuously for four hours (with one 20 minute break) (Snook & Ciriello, 1991). Subjects were 10 male and 12 female industrial workers performing 18 various lifting, lowering, pushing, pulling and carrying tasks at frequencies of 4.3 per minute or less. The third experiment also reviewed a combination task consisting of a lift, carry and lower. It was noted that previous Liberty Mutual experiments have investigated work elements, such as lifting, in isolation. This addendum to the third experiment followed the same methodology as that prescribed for the work tasks reviewed in isolation (Snook & Ciriello, 1991). The fourth experiment investigated tote boxes without handles, and lifting with extended reaches. Subjects were six males. Forty-two variations of lifting, lowering, pushing, pulling and carrying tasks were performed. Methodology followed that of previous three experiments.

Results of the four additional experiments which were designed to fill-in previously assumed tabular values indicated general accuracy in assumptions save for forces and weights at lower frequencies (Snook, 1978; Snook, 1985; Snook & Ciriello, 1991). It was found that the

weights and forces for the 5 minute and 30 minute task frequencies were overestimated in the original table by 10 to 15% (Snook, 1978; Snook, 1985; Snook & Ciriello, 1991). Further and importantly, the average values of maximum acceptable weights and forces for the very high frequency tasks (tasks faster than 4.3 per minute) were associated with oxygen consumption values that exceeded the physiological criteria for an 8 hour work-day (33% VO₂max) (NIOSH, 1981; Snook & Ciriello, 1991).

The addendum to the third and fourth experiments indicated that a combined task of lift, carry and lower resulted in significantly lower maximum weights and forces than that of a carry task in isolation. This was not the case for lifting or lowering where they were not significantly different. Results from experiment two and four indicate that horizontal grip distance from the body and task distance and height are significant variables to consider while establishing manual handling guidelines (Snook, 1985; Snook & Ciriello, 1991). Specifically, the fourth experiment found that when horizontal reach is extended (480mm) as compared to close to the body (170mm), results indicate a median decrease in acceptable weights and forces of 48% (Snook & Ciriello, 1991). It is noted that the biomechanical modeling of NIOSH (1981) and Chaffin & Andersson (1984) confirm these findings (Snook & Ciriello, 1991).

The fourth experiment discovered that boxes without handles (poor coupling) resulted in a consistent and significant decrease in acceptable weights and forces. These values varied with frequency of action and box size. The median decrease was 16% (Snook & Ciriello, 1991). The fourth experiment also found significant differences in maximum acceptable weights and forces between pushing and pulling tasks over longer distances (15.2m). The maximum acceptable initial force for the pulling task was 13% lower than for the pushing task. Further, the respective maximum sustained force was 20% lower (Snook & Ciriello, 1991).

The results of the original seven studies were integrated with the results of the supplementary four to establish a master eleven (Snook, 1978; Snook 1985; Snook & Ciriello, 1991). Each of these eleven experiments included two types of tasks: criterion and variation tasks

(Snook & Ciriello, 1991). Each experiment investigated different variations in task frequency, height, distance and box size. With the vast number of possible combinations and permutations, the researchers stipulated that it was impractical to run every subject through all variations (Snook & Ciriello, 1991). They decided to utilize the percentage difference from the criterion task to develop an adjusted mean for each variation task. The standard deviation for each variation task was then determined from the adjusted mean and the criterion task coefficient of variation. With these values (mean and standard deviation for criterion and variation tasks) and statistical normal distribution data, the maximum weights and forces acceptable to 10, 25, 50, 75 and 100% of the industrial population were derived (Snook & Ciriello, 1991).

2.3.1.1 Limitations & Assumptions of the Liberty Mutual Tables

Many of the limitations and assumptions involved with the Liberty Mutual tables are artifacts of the experimental and statistical methods used. The psychophysical analysis technique relies on the subject(s) to monitor and provide feelings and perceptions with regard to exertion and fatigue. There may be number of psychological factors which will have an effect on the psychophysical response during the manual materials handling activities involved in these experiments. Many of these may be found in tabular format in Mital et al. (1993).

Since all variables (other than the one being freely adjusted by the subject(s)) must be controlled for, the psychophysical methodology is typically restricted to laboratory investigations (Mital et al., 1993). The results of these experiments are specific to a tightly controlled situation, thus transference to the industrial workplace requires some flexibility with assumptions. For example, the Liberty Mutual tables are designed to provide safe effort levels for work up to 8 hours, five days a week with a standard break schedule (Snook et al., 1970; Snook and Ciriello, 1991). Many of today's modern manufacturing firms require employees to work for 10 or more hours per day, 6 (or more) days per week. The Liberty Mutual tables do not have a decreased value for extended working periods. Thus, individuals who wish to apply the data from the tables

in these environments must apply some rule-of-thumb techniques to compensate for extraneous factors.

Naturally there will be broad variations in population strength as is implicit to normative statistics. This must be countered with sufficient sample size. The Liberty Mutual research tended to use relatively large sample sizes (15 to 59 subjects) for its criterion tasks (Snook, 1978; Snook & Ciriello, 1991), however the number of subjects used in the variation tasks were well short of the criterion (≤ 12 female subjects for each supplementary experiment)(Snook, 1985). It should be noted that the percentage difference between criterion and variation task was used to develop the adjusted mean for each variation task. Further, the standard deviation for each variation task was derived from the aforementioned adjusted mean value and the criterion task coefficient of variation. Since the variation tasks had relatively small sample sizes, there may have been a significant impact on the prescribed values. A basic tenant in statistics is that the larger the sample the better (Leedy & Ellis, 2001). It has been stipulated that sampling error is likely to occur while using parametric statistical techniques, where the sample size is less than thirty (as was the case with the Liberty Mutual variation experiments) (Gravetter & Wallnau, 1988). Further, it is stipulated that assumptions had to be made to fill-in specific variations that had not been studied. The values were developed based on 'adjustments' developed from the closest applicable studied value. For example, Variations in frequency and distance for pulling tasks are based upon adjustments developed for pushing tasks (Snook & Ciriello, 1991).

It is assumed that an individual who is to apply the values from the tables has read and understands that certain reductions in weights or forces should accompany deviations from an ideal state. For example, Snook and Ciriello (1991) stipulate values for handling tote boxes without handles should be reduced by approximately 15% from the tabular value. Further, when handling smaller boxes with extended horizontal reaching between knee and shoulder heights the tabular values should be reduced by 50% (Snook & Ciriello, 1991).As evidenced by the large

multiplier values, these subtleties may contribute significantly to the outcome from an industrial task design perspective.

The practitioner should be knowledgeable enough to apply the tabular values in circumstances where the prescribed weights and forces are most applicable. For instance, at low frequencies (one lift every 5 & 30 minutes) of manual materials handling, the psychophysical method may overestimate physical capabilities (Mital et al., 1993). It should be noted that this bias was thought corrected-for in later publications (Snook, 1985; Snook & Ciriello, 1991).

Comparative results derived from a biomechanical modeling tool versus the Liberty Mutual tables (1991) for the same elements of several operations indicate that the most recent psychophysical tables still overestimate physical capabilities at very low frequencies. Also, at high frequencies it was observed that the psychophysical technique produces overestimates of maximum acceptable weights and forces (Ciriello & Snook, 1983; Fernandez et al., 1991). In fact, the average values for the very high frequency tasks (tasks faster than 4.3 per minute) were associated with oxygen consumption values that were greater than the accepted criteria for an 8 hour day (Snook & Ciriello, 1991; NIOSH, 1981). These results are supported by similar experimental findings where high frequency lifting (above 6 per minute) may cause the subjects to misjudge acceptable values because they are cuing on muscle tension instead of metabolic demands (Karwowski & Yates, 1986). The findings indicate that the use of the table values for manual material handling should be restricted to relatively low to moderate frequencies (Snook & Irvine, 1969; Karwowski & Yates, 1986).

2.3.2 Biomechanical Approach in EDS

The science of biomechanics provides the basis for certain strength prediction models. The biomechanical model breaks the body into segments, each having a mass as determined through anthropometric studies (Eastman Kodak Company, 1986). These models may be (and are often) designed to assess the forces acting on particular articulations and identifying potentially hazardous working conditions (Chaffin and Andersson, 1991).

A strength prediction model that is commonly used is the University of Michigan's Three Dimensional Static Strength Prediction Program (3DSSPP™). This model may be used to simulate a wide variety of working postures and allows for a variety of anthropometric populations to be reviewed. The model is useful for the analysis of forces acting upon the body under 'slow' moving conditions with 'heavy' materials handling tasks (University of Michigan, 2000). The tool may be used to analyze symmetric and asymmetric postures. Further differing magnitudes of hand forces for the left and right hands can be entered and may act in common or differing directions. The model requires certain inputs including worker anthropometric characteristics, worker posture while exerting force, and the load in the hands and the direction of application. With these inputs the model is able to provide the compression force realized by the back (comparative with NIOSH limits), the strength requirements for each joint, the percentage of the given population capable of completing the task and the required coefficient of friction at the shoe – floor interface. These values are based upon a large database of isometric strength data collected over a 25 year period.

2.3.2.1 Limitations and Assumptions of the Biomechanical Approach

As mentioned in an earlier section of this document, the biomechanical approach (generally used as a low-frequency component of the integrative approach) is used to estimate the mechanical stresses on the body while performing some task. Within these models the human body is divided into a series of linked segments, each possessing a similar length, center of gravity and mass to those of the population being studied (Loslever & Ranavoisa, 1993). Limitations inherent to the biomechanical approach include, the complexity of the human body and the translation of complex joint interactions to mathematical modeling (Park, 1973). Researchers attempt to counter these limitations with model scope and sophistication designed to increase the accuracy of results. The unfortunate outcome of this increased specification is that the models become only applicable to very narrow situations and do not translate well to other tasks (Armstrong et al., 1979; Jagger and Luttman, 1989).

Biomechanical models vary in the number of articulations and vascular and non-vascular tissue interactions. Cadaver, biopsy and animal studies are used to identify the complex physical interactions and properties of a particular segment of the human body (Goldstein et al., 1987; Dennett & Fry, 1988; Topp & Byl, 1999). Further, complex electronic equipment, such as electrogoniometers, accelerometers and electromyography are commonly utilized to identify joint dynamics and tendon travel (Kadefors et al., 1976; Silverstein, 1985; Silverstein et al., 1987; Schoenmarklin & Marras, 1993; Deal, 1995; Marras et al., 1995; Sommerich, 1996; Potvin, 1997). Obviously with each physical study and with the use of these varied and often complicated devices, the possibility for bias and technical error increases. The combination and application of the knowledge obtained from these studies assumes that the studies were well performed and that all care was taken to control for potential sources of informational noise (Fisher et al., 1993).

Biomechanical models are generally designed to take into account various amounts of information, compute the forces acting on a joint and then compare those against some ultimate tensile or compression value. The validity and reliability of the comparator is then essential to accurate outcomes. For example, in reviewing several studies, Mital et al. (1993) found a range in ultimate compressive force from 3000N to 12,000N. It was further found that several demographic and physical characteristics play a significant role in the compressive forces. These too must be accounted (or acknowledged). Even with all of this available information, in order to effectively estimate the mechanical stress imposed upon the body while performing dynamic or static work, a number of simplifications and assumptions concerning segment and tissue interaction are necessary. The nature and extent of these assumptions and simplifications determine the sophistication of the biomechanical model (Mital et al., 1993).

The 3DSSPP™ model (as discussed previously) is designed to assess a variety of manual handling tasks and represents a culmination of decades worth of research. The model was scrutinized by Chaffin and Erig (1991) during a study which collected data from 29 male subjects

during a lift and three push and pull tasks. Results indicate that the model is highly sensitive to slight alterations in posture. The user must be aware of the potential for significant differences in outcomes with minor data input changes. The 3DSSPP™ model was developed from isometric data collected over several years. As such the model is intended to be used for slow, gross movements which are not common in the contemporary industrial environment. As such the user must be able to scale the model output by balancing inputs between applicable population gender, anthropometry and percent strength capable. Further multiplier values should be used to adjust outputs for frequency.

2.3.3 Physiological Approach in the EDS

Careful manipulation of metabolic equations can allow individuals to determine energy expenditure as the result of lifting, lowering, pushing, pulling and/or carrying a specified load. This then may be compared to an individuals maximum aerobic power (MAP) in order to provide a relative ratio of energy used to energy available. Garg (1976) and Garg et al. (1978) used this reasoning toward the development of the metabolic equations.

The metabolic equations as proposed by Garg (1976) were founded upon the findings of Snook (1969). These studies indicated that a design criteria of 33 percent MAP would be protective for most workers. Within these studies, 16 kcal/min was taken as MAP for healthy, young males during a dynamic job. Chaffin (1967) stipulated that 5.2 kcal/min should be sufficiently protective for young males averaged over an 8-hour working day. This value is based on 33% of 16 kcal/minute. However, Garg et al. (1978) stipulate that women and older workers require a much-smaller physical work capacity limit. Garg (1976) surmised that from a review of the available methods, a better and more applicable predictive model was required. Further, it was stated that any physiological fatigue criteria (i.e. 5.2 kcal/minute) cannot be used by the work analyst unless converted into useful design parameters such as frequencies, weights, distances and more (Garg et al., 1978).

The purpose of this study was to develop a method for estimating the metabolic energy expenditure rate based on physical descriptions of a job and the worker completing the job tasks. This method was to be designed to maximize usefulness within the industrial environment (Garg et al., 1978). The model itself was based on the assumption that a job can be divided into simple task elements and that the mean metabolic energy expenditure rate of the job can be predicted by knowledge of the energy expenditure of the tasks and duration of the job. The model uses the calculation that the mean metabolic energy expenditure equals the sum of the energy used for each task plus the energy used to maintain a particular body posture averaged over the time of exposure (Garg, 1976). In order to establish baseline net metabolic cost for various elements of the equation a systematic collection of metabolic energy expenditure rate data for 28 separate tasks was undertaken in a laboratory setting. Over 540 oxygen uptake measurements were made. Differing levels of weight of load (force) and frequency of loading the body (pace) were employed for each task. The experiments were designed so that the main effects and some interactions accounting for the majority of the variation in the energy expenditure rate could be analyzed.

Prediction equations of net metabolic cost for each task as a function of personal and task variables were developed. It is stated to be of importance to note that gender effects appear for certain tasks (lifting, lowering, pushing at bench-height, lateral movement of arms of 90 degrees) but not for others (holding, walking, carrying, forward movement of arms, lateral movement of arms 180 degrees) (Garg et al., 1978). Further it is said to be worth mentioning that the prediction equations are presented as net metabolic cost per performance. Therefore, these equations can also be used to estimate the net metabolic cost of infrequently occurring tasks or elements that appear in special cycles of a repetitive job. However the metabolic equations do not cover small hand or arm movements (i.e. cutting or cranking) (Garg et al., 1978).

Chaffin (1967) developed a prediction model for the metabolic energy expended during arm activities. The model was primarily limited to weight holding activities in the sagittal plane.

The net metabolic rates for holding 4.5, 13.6 and 22.7kg loads against the waist by a 75kg seated subject were reported as 0.22, 0.71 and 1.66 Kcal/minute respectively. The corresponding values as derived by Garg (1976) were 0.28, 0.84 and 1.40 Kcal/minute. The differences between the two studies results were attributed to inter-subject variability in net metabolic costs (Garg et al., 1978).

A comparison between the values derived by the Garg (1976) equations and those proposed by Snook (1971) for lifting tote boxes was reported. Results of the lifting comparison indicate that the total metabolic rates as predicted by Garg (1976) are comparable to the means of the measured metabolic rates (Garg et al., 1978). The average absolute difference was 6.8 percent. It was noted that the predicted metabolic rates for lifting were consistently lower than the means of the measured metabolic rates. This was explained to be attributable to the fact that the body weight used by Snook (1971) was not representative of the industrial working population, and that if 91kg (rather than 77kg) was used, the predicted rates would be consistently higher than those measured (Garg et al., 1978).

In conclusion, the research indicates that the metabolic rate prediction model can be used to estimate metabolic rates for a wide variety of manual materials handling jobs. The partitioning of a job into its component elements allows for the identification of those tasks that are particularly taxing to the worker. This model was said to be useful in the design of industrial operations (Garg et al., 1978).

2.3.3.1 Limitations & Assumptions of the Garg Metabolic Equations

Physiological studies are subject to their own limitations and assumptions. These studies review an individuals (or groups) physical endurance and limitations, considering the physical demand for oxygen and nutrients and the disposal of waste by-products. There are several measures which may be used to assess the efficiency of the system, some of these include, metabolic energy cost, heart rate, blood pressure, blood lactate and ventilation volume (Mital et al., 1993).

Each of these techniques differs in their respective invasiveness, and each require careful and considerate analytical methods.

Typically, metabolic energy expenditure has been the most widely used technique to assess repetitive materials handling as it is directly proportional to the workload at steady-state conditions (Mital, 1984a; Astrand & Rodahl, 1986). There are several contributory factors which effect metabolic energy expenditure rate. Each of these positively or negatively impact muscle recruitment which in-turn directly impacts energy cost. Metabolic energy expenditure is dependant upon the amount of muscle groups active during task performance (Mital et al., 1993; Kilbom, 1994b). All of these factors must be acknowledged within research methodology or addressed within the assumptions or limitations of the work.

With regard to Garg's equations (1976), the first and obvious limitation study was the use of only six subjects. Such a small sample size makes statistical significance difficult to establish and allows data anomalies or spurious elements to have a large effect on data analysis. Further, the subsets of subjects (gender, weight) which were used to establish multiplicative effects for energy expenditure are suspect due to the small sample size of each (i.e. 3 male; 3 female). The experiments were performed within a laboratory setting which findings, it may be argued, are difficult to transfer reliably into the industrial environment. The strict controls required of the experiment each serve to call into question the application to another less-controlled setting. For example, the tote box was controlled for size and coupling where industrial manufacturing often requires the manual manipulation of multiple items with varying dimensions, frictional properties and load stability. Unless controlled-for, each assumption decreases the validity of the tools results in an industrial setting. An additional limitation of the study was that the subjects performed tasks for far less time than would be required of a typical manufacturing assembly job. In fact, it is stated that experiments were performed for only ten minutes. It is explained that the first five minutes were used to establish a steady heart rate, where the subsequent five were recorded for ventilatory minute volume and the oxygen content of expired air.

2.3.4 Integrative Approaches in EDS

Mital Tables: Recognizing that none of the individual research approaches can provide 'safe' load recommendations across the entire range of frequencies (Mital, 1985; Mital et al., 1987; Mital, 1992), Mital et al. (1993) developed an integrative method to determine what would be deemed as a physically 'safe' load for a worker to lift, lower, push, pull or carry over a variety of postures, frequencies and durations. As integration implies, the tables make use of a combination of biomechanical, epidemiological, psychophysical, and physiological disciplines. The ultimate goal of this composite approach is to use the 'most significant task factor', namely frequency, to determine which prescribed value would be most applicable in a given materials handling situation (Mital et al., 1993). As with the Liberty Mutual tables, gender, population percentiles, box size or handle height and physical ranges further refine choice variables to the most appropriate value. The design criteria, effectively a scalable safety threshold value 'which must not be violated' was established for each of the four approaches and each of the physical actions (Mital et al., 1993). This criterion value was based on the premise that injury severity and incidence rate increase almost three-fold as job requirements approach the strength limits of workers (Chaffin et al., 1978).

For the lifting element, previously established psychophysical data (Snook, 1978; Snook & Ciriello, 1991) were used as the base. The rationale is that this data provides design criteria across almost the entire lifting frequency range. This database was modified in regions where the biomechanical or physiological design criterion were the limiting factors (Mital et al., 1993). The design criteria for lifting based on the epidemiological approach utilized the research of Ayoub et al. (1983) and Ayoub and Mital (1989). The studies established a 'Job Stress Index' (JSI) which is a working duration, lifting frequency, load and lifting capacity based index (Ayoub & Mital, 1989). A 'critical JSI value' of 1.5 was set. That is to say that the occurrence of injuries, illnesses and the severity of these increased substantially when this index was exceeded (Ayoub et al., 1983). The study included mostly male participants and the weight equitable to a JSI value of 1.5

was 27.24kg. The compressive value associated with the JSI value of 1.5 is based on the three dimensional biomechanical model of Kromodihardjo and Mital (1986, 1987) and is approximately 3930N. This represents 69% of the mean ultimate compression strength established by Jager and Luttmann (1991). Mital et al. (1993) equate this percentage to the female population to establish a spinal compression limit of 2689N. This would correspond to a weight of 20kg, and a JSI held at 1.5. Therefore the biomechanical limits for use within Mital et al. (1993) composite approach would be approximately 27kg for males and 20kg for females, such that any table values higher than this would be replaced by these load magnitudes.

As discussed previously, the physiological approach is not limiting due to load but rather the endurance of the individual. As one may assume, the combination workplace risk factors will significantly increase the rate of expenditure. Further, it should be noted that the primary reason for the sensitivity of metabolic energy expenditure rate to workplace risk-factors is the fact that energy cost is dependant on the number and size of muscle groups recruited to perform a task (Mital et al., 1993; Kilbom, 1994b).

It has been determined that occupational tasks requiring a metabolic energy expenditure of more than 5 kcal/minute (approximately 33-35% of treadmill aerobic capacity) will lead to overexertion and undue fatigue (Michael et al., 1961; Bink, 1962; Mital et al., 1993; Sanders & McCormick, 1993). Some studies have indicated that a limit of 33% maximum aerobic power (MAP) will be protective of workers for an 8-hour workday. Knowing that the MAP for healthy young adult males is about 15 kcal/minute, one third of this is 5 kcal/min (Sanders & McCormick, 1993). Others have stipulated that this value is too high and that a more conservative approach is required. Frederick (1959) suggests that energy expenditure for an 8-hour workday should not exceed 3.33 kcal/minute.

Further studies indicate that when frequencies are above 4 lifts per minute, the psychophysical and physiological approaches provide very similar weight recommendations. When frequencies are at, or below, 4 per minute, psychophysical recommendations should be

considered more valid (Mital, 1985). It should be noted that while comparing load recommendations for lifting activities, Garg and Ayoub (1980) found that the psychophysical design criteria leads to greater work loads at higher frequencies when compared with the physiological approach. Further, while lifting from floor to 0.51 meters in height, the frequency threshold of 6 per minute was the point at which the physiological criterion limit was exceeded, indicating that the physiological analysis technique is more appropriate at higher activity rates

The ultimate result of the integrative approach used by Mital et al. (1993) are a series of look-up tables (as Snook & Ciriello, 1993) which provide ergonomically safe values for both genders over many manual materials handling tasks seen in industry today. In order to use these tables effectively, one reviews the action options (Lift/Lower, Push/Pull, Carry) and locates a safety value based on work constraints from the appropriate table. One key feature to this compilation is the availability of correction factors which are designed to address certain information gaps which would likely have an impact on the safety margin for that task. These correction factors consist of multipliers which may be applied to the tabular values. All correction factors were designed to be used for lifting and carrying conditions. The work duration correction may effectively be applied to all manual materials handling actions. These correction factors may be found in Mital et al. (1993).

NIOSH Lifting Equations: The integrative approach was also used by the National Institute for Occupational Safety and Health (NIOSH) (1981) while establishing a work practices guide for manual lifting. An equation was developed based on the design criterion for biomechanical, psychophysical and physiological methodologies. The formula was comprised of the critical elements required for ergonomic analysis within which manual lifting tasks are characterized by variables including frequency, part weight, spatial factors and duration (Reed et al., 1999). In 1991, this equation was modified to address some of the original limitations and now included a lowered initially acceptable weight (23kg rather than 40kg as 1981) and multipliers for asymmetrical lifting, twisting and object coupling (Waters et al., 1993). The alteration in the load

constant represents both a desire to decrease the load constant but also a perceived need to increase the horizontal displacement component of the equation from 15 to 25cm. With the horizontal correction, the seemingly large change in the load constant represents only a 1kg reduction from the 1981 equation (Reed et al., 1999). These alterations were prompted by new research and reflect changes in psychophysically determined findings as established by Snook and Ciriello (1991).

The biomechanical aspect of the equation required prescribed inputs to provide a value which could estimate compressive forces on the low back, the value attained could then be compared to established thresholds for safe lifting based on maximum disc compression (Chaffin & Park, 1973; Jager & Luttman, 1989). The result was a cut-off value of 350 kg of disc compressive force centered on the articulation between the fifth lumbar and first sacral vertebrae (Waters et al., 1993). This location was chosen as the site of greatest lumbar stress during lifting (Ayoub and Mital, 1989; Waters et al., 1993).

In order to address repetitive lifting the NIOSH 1991 committee selected metabolic energy expenditure as the criterion measure. The committee attempted to prevent muscular fatigue, which is likely to accompany high-frequency repeated lifting, by establishing a baseline maximum aerobic capacity (Waters et al., 1993). It was decided that the capacity of 9.5 kcal/min or 4000 kcal per standard working day (420 minutes) would serve as the threshold value. The baseline energy expenditure was 10.5 kcal/min which was discounted to 9.5 kcal/min due to concerns that treadmill tests overestimate maximal aerobic capacity for repetitive lifting (Reed et al., 1999). This criterion is supported by many studies (Astrand & Rodahl, 1977; Mital, 1984a ; Karwowski & Yates, 1986), however the main contributor is the research of Rodgers et al. (1991). It should be noted that the NIOSH 1991 committee stipulates that more research is required to validate the physiological aspect of the equation for paced lifting, such as that required of assembly line operations.

The NIOSH 1991 committee made adjustments to the physiological capacity value in order to address initial vertical lifting location (surrogate measure of body parts involved) and durations for repetitive lifting. A threshold was established for initial vertical height of lift of 75 centimetres . The committee reasoned that any initial vertical position below 75 centimetres required the use of the muscles of the whole body. Lifts initiating above 75 centimetres required primarily the shoulder and arm muscles. It was further stipulated that primarily arm lifts require and expend less energy than whole body lifts. However, the capacity of those muscles was also significantly less. In order to adjust for lifts above the 75 centimetre mark, the 1991 committee implemented a 30 percent reduction in the energy expenditure limit of 9.5 kcal/min.

Three durations were utilized to adjust for muscular aerobic energy expenditure within the NIOSH (1991) equation. For durations one hour or less, the figure of 9.5 kcal/min should be reduced by 50 percent. Durations greater than one hour up to two hours the value should be reduced to 40% of the original. For repetitive lifting tasks requiring more than 2 hours up to and including 8 hours the value of 9.5 should be reduced by 66 percent. Using baseline criteria derived from biomechanical, physiological and psychophysical research, the individual components of the 1991 NIOSH lifting equation were developed. It is stated that each component of the revised lifting equation was designed to satisfy these criteria. Where conflicting results arise, the most conservative approach was taken (Waters et al., 1993). Each individual element and the resulting input into the 1991 equation are discussed below.

The horizontal multiplier (HM) is dependant on the vertical height at the start of the lift (< or > than 25cm) and the box width. This logic was supported as Potvin and Bent (1997) found a significant relationship between horizontal hand location, box width, and initial vertical height of the lifting task. The vertical multiplier is defined by the vertical distance of the hands to the floor (Vi, 1998). The multiplier values were determined by reviewing psychophysical, epidemiological and biomechanical data over a variety of heights. The determination of the vertical multiplier was more complicated because it varies over all vertical heights, not just for

two ranges (Reed et al., 1999). The results set by the 1991 committee was a reduction of at least 22.5% in allowable weight for lifts originating near the floor (Waters et al., 1993). Empirical data derived from the research of Snook (1978), Ayoub (1978) also Snook and Ciriello (1991) were used to establish the discounting value of 22.5% for lifts above 150cm. The distance multiplier (DM) is defined as the vertical travel distance between the origin and the destination of the lifting/lowering task (Vi, 1998). The NIOSH 1991 committee reviewed several research papers which indicated that lifting at or near spatial limits (reach zone, floor to above shoulder) results in a 15% decrease in the maximal acceptable weight of lift (Waters et al., 1993). Asymmetrical angle is defined as the angular measure of how far the object is displaced from the front (mid-sagittal plane) of the workers body at the beginning and end of lift (Vi, 1998). Reviewing biomechanical and psychophysical data on asymmetrical lifting revealed a decrease in maximum acceptable weight by 8 to 22 percent as asymmetry increases (Waters et al., 1993). Further, there is evidence of a decrease in isometric lifting ability by 39% with lifting tasks at 90 degrees as compared to symmetric lifting (Waters et al., 1993). Coupling describes the quality of the grip between the hand and the object (Vi, 1998). Loads equipped with appropriate couplings or handles facilitate lifting and reduce the possibility of dropping the load (Waters et al., 1993).

In reviewing several psychophysical studies it was established that the reduction in lifting capacity due to poor coupling should be in the order of 7% to 11%. Frequency of lift is defined as the average number of lifts or lowers made per minute (Vi, 1998). For use within the 1991 equation, the frequency multiplier (FM) was expressed as a value within a table rather than a formula. The Liberty Mutual values as derived from the research of Snook and Ciriello (1991) were used for lifts at 4.3 lifts (effectively 4) per minute and below. As discussed, the 1991 equation consists of an initial load constant (23kg), multipliers for each task variable are then applied. The result is the recommended weight limit (RWL). The data of Snook and Ciriello (1991) (MAWL) were substituted for the RWL at < 4 lifts per minute. The 1991 committee selected a psychophysical criterion designed to ensure that job demands would not exceed the

acceptable lifting capacity of 75% female workers or approximately 99% of male workers (Waters et al., 1993). For frequencies exceeding 4 lifts per minute, the equations developed by Garg (1976) were used. The resulting weights were used to determine frequency multipliers by dividing each into the load constant. Finally, the 1991 committee adjusted the original multiplier values to provide a close approximation of observed and predicted effects of lifting frequency on acceptable workloads for lifting (Rogers et al., 1991; Waters et al., 1993). It should be noted that tabular values are provided by NIOSH (Waters et al., 1993) at durations of < 1 hour and < 2 hours, but for use within the EDS, the values of 2-8 hours are used as representative of typical working conditions within the automotive assembly facilities.

2.3.4.1 Limitations & Assumptions of Integrated Approaches

As the name implies, integrated approaches make use of several research techniques and are therefore inherently subject to the limitations and assumptions of each. The limitations of the psychophysical, biomechanical and physiological approaches were well documented in their respective reviews, therefore will not be repeated here. With regard to manual materials handling, the epidemiological research approach attempts to identify symptomological patterns which may then be used to preempt future occurrences of similar movement or effort patterns. This approach relies heavily upon accurate and comprehensive recordkeeping, tracking incidences, injuries and illnesses and/or honest feedback of fatigue and discomfort from test subjects (Yoshitake, 1971; Mital et al., 1993). A review of epidemiological studies indicates that much of the information linking workplace risk-factors and injury or illness is lacking or only a qualitative link (Frymoyer et al., 1980; Troup et al., 1981; Damkot et al., 1984; Stock, 1991; NIOSH, 1997). Also, many of the studies suffer from small sample size, lack of adequate control, are conducted for short periods and are retrospective (Mital et al., 1993). Dealing with subjective information, such as complaints of low back pain, which frequently may be unreliable is another major shortcoming of epidemiological studies (Glover, 1970). Very few risk factors have been definitively linked to injuries using epidemiological research (Mital et al., 1993).

There are several limitations and assumptions with regard specifically to the utilization of the NIOSH lifting equation. These have been set forth by the 1991 NIOSH committee themselves and are to be used as guides for both the proper and intended use of the equation and to emphasize the requirements for future research. Waters et al. (1993) stipulate that the design criteria based on biomechanical, physiological and psychophysical design criteria should be reviewed and adhered to. Further as mentioned previously, limitations inherent to each apply. The 1991 committee acknowledges the need for the equation and its components to be validated. Several studies have recently attempted to do just that. We will review these and their respective conclusions as they apply to the limitations and assumptions of the 1991 NIOSH lifting equation (NLE).

The frequency distribution and validity of the 1991 NIOSH recommended weight limit (RWL) were studied by Vi (1998). It was indicated that little is known about the practical implications of the RWL under real-world situations and that few studies have attempted to validate this. The purpose of the study was to compare the internal validity of the RWL with established psychophysical data under a variety of scenarios using a Monte Carlo uncertainty analysis. Simulations of 64,000 lift/lower conditions were run within the boundaries of each element range specified in the paper (Vi, 1998). The NLE (1991) was deemed to be a conservative tool where 99.9% of the 64,000 scenarios were protective for 99% of the male population (Vi, 1998). This leads one to enquire about the sensitivity of the tool at its proposed threshold limit value. If the tool exhibits poor sensitivity an unacceptable level of false positives will result (Joseph et al., 2000).

Citing the fact that little information exists about the NLE ability to predict incidence and severity of lower back disorders due to the lack of epidemiological data, Dempsey et al. (2000) proposed a field evaluation of the revised NIOSH lifting equation. The goal of this study was to investigate the relationship between the 1991 NLE and the incidence and the filing of workers

compensation claims. Second, they sought to evaluate the usefulness of the tool in a variety of work settings (Dempsey et al., 2000).

Due to the extreme difficulty finding jobs which met all of the criteria for the 1991 NLE, the methods employed in this study required the relaxation of the NLE protocol on extraneous manual materials handling elements (push, pull, carry), with these tasks then to be assessed with psychophysical data. Jobs for inclusion within the study were required to be primarily lifting and lowering intensive, however not exclusive (Dempsey et al., 2000). Outcomes measures were derived from OSHA 200 logs and workers compensation claims during follow-up periods. Results were obtained from the baseline assessments of 362 subjects of more than 60 facilities that took part in the validation study. Of the initial 362 subjects, there were 180 follow-up respondents. Dempsey et al. (2000) stipulate that a history of low back pain was the most consistent risk factor found. Summary statistics indicated a mean weight of 11.7 kg for the 1123 lift or lower tasks observed. The conclusions drawn from this study were that there was not enough epidemiological data to conclusively determine the validity of the NIOSH lifting equation. It was also noted that since the NIOSH equation is designed solely to analyze lifting and lowering, it is restrictive in an industrial setting that requires many manual handling activities (Dempsey et al., 2000).

Reed et al. (1999) decided to review the frequency factor in manual lifting by analyzing that component of the 1991 NLE. The stated purpose for doing this was due to the fact that many individuals of varying credentials are charged with the ergonomics responsibilities within a business. Many of these ergonomists have limited knowledge with regard to the background, limits and assumptions of the resources (as the NLE) that they use. Through this research it was concluded that by first deciding on spatial multipliers, estimates for frequency result in values that are more conservative than research can support. Further, data show that the new version is far more conservative than the previous (1981) equation with the frequency and horizontal multipliers playing key roles (Karwowski & Brokaw, 1992; Vi, 1998; Reed et al., 1999). The

threshold limit value as proposed should be scrutinized to adjust for the inherent conservative nature of the tool.

2.3.5 Electromyography (EMG) in EDS

Electromyography (EMG) has been used extensively to evaluate muscle activity (Kadefors, Peterson. & Herberts, 1976; Armstrong, Chaffin & Foulke, 1979; Herberts, Kadefors & Broman, 1980; Hagberg, 1981; Habes, Carlson & Badger, 1985; Suurkula & Hagg, 1987; Giroux & Lamontagne, 1992; Wells et al., 1994; Hagg, Oster & Bystrom, 1996; Potvin & Bent, 1997; Potvin, 1997). EMG is a technique used to indicate when muscles are active and the relationship between a level of activity and the worker's capacity.

Worker capacity is difficult to establish as one may imagine. Controlled experiments where subjects work until injury or illness occurs is obviously not acceptable. Another means to predict a potentially injurious condition was required. It has been a widely accepted assumption that musculoskeletal injuries are preceded by localized muscle fatigue (Yoshitake, 1971; Herberts, Kadefors & Broman, 1980; Hagberg, 1981; Borg, 1982; Habes, Carlson & Badger, 1985; Waly, Kahlil & Asfour, 1986). While the exact relationship between fatigue and injury has not been clearly established, there is consensus among researchers that fatigue plays an important role (Baidya & Stevenson, 1988; Baron, 1996; Yamada, Kiryu & Okada, 2001). Muscular fatigue therefore is viewed as an ethically-driven surrogate measure of risk and task design to avoid fatigue is seen as a rational method to minimize this risk (Yoshitake, 1971; Merletti et al., 1991).

Fatigue may be defined simply as the inability of an individual to continue with a particular physical activity at a steady intensity (DHHS, 1992). Though difficult to analyze in the field, subjective and objective methods have been proposed. Psychophysical rating scales, such as the Borg (1982) scale may be used to document the workers perception of fatigue. Alternatively physiological methods such as electromyography (EMG) may be used to quantify fatiguing conditions. The most common measure of fatigue is the use of EMG to measure the

subjects capability versus the subjects maximal voluntary contraction (MVC). This technique has been dubbed the "gold standard" for the identification of fatigue occurrence (Vollestad, 1997).

Muscle fatigue may be identified through the use of EMG by observing alterations in the spectral characteristics of the myoelectric signal. It is well-documented that the power spectrum of surface EMG shifts toward lower frequencies and its magnitude increases as muscle fatigue progresses (Christensen, 1986; U.S. Department of Health & Human Services, 1992; Yamada, Kiryu & Okada, 2001). The changes have been attributed to increased muscle motor unit recruitment in response to high level contractions compressing blood flow in the muscle, aerobic metabolism changes to anaerobic due to resulting acidosis, muscle fiber conduction velocity decreases due to decreased pH in the muscle and changes in the shape of the action potential shifts the power spectrum (DHHS, 1992; Yamada, Kiryu & Okada, 2001).

In using electromyography to evaluate risk, three levels of muscle loading have been of concern for ergonomists, those being peak, dynamic and static. Bengt Jonsson (1982) defines these three levels based on the amplitude probability distribution function (APDF). The APDF is the distribution of the levels of muscle contraction during an observation period (Ankrum, 2000). Jonsson goes on to specify a quantity of time that may be 'safely' spent at a given contraction level (% MVC). Peak load level, effectively the highest level of muscle activity during the EMG recording, is defined by Jonsson (1982) as the 90th percentile value of the APDF. The dynamic load level is deemed the 50th percentile and the static load level for muscle activity is defined as 10% or below. Jonsson (1982) established physical threshold values based on these work durations. He stipulated that a worker should not expend more than 2-5%, 10-14% and 50-70% of maximum voluntary contraction (MVC) during static, dynamic and peak work durations respectively (Wells et al., 1994; Ankrum, 2000). For example, to remain within Jonsson's (1982) threshold limits, a workers static level of muscle activity would have to remain at or below 2-5% of EMG recorded MVC for 10% of the time or less (Wells et al., 1994).

2.3.5.1 Limitations & Assumptions of EMG-Based Methods

The quantitative threshold values as established by Bengt Jonsson (1982) which are used to analyze EMG signals and interpret physical stress levels have been cited frequently in the analysis of occupational risk factors (Aaras & Westgaard, 1987; Aaras, 1994; Wells et al., 1994; Ankrum, 2000). Jonsson (1982) suggests that the 90th percentile maximal voluntary contraction (MVC) of the amplitude probability distribution function (APDF) (which he calls 'peak') should not exceed 50-70%. The 50th percentile (which Jonsson calls 'dynamic') should not exceed 10-14% and the 10th percentile (called 'static') should not exceed 2-5%.

Wells et al. (1994) stipulate that guidelines for the 'static' condition as established by Jonsson (1982) may be too high to prevent chronic injury in the shoulder musculature. Ankrum (2000) suggests rather that there is simply confusion in the terminology. He stipulates that the confusion arises due to the similarity between the terms 'static task' and 'static load level'. Ankrum (2000) states that a 'static task' is a loosely defined reference to work in which muscles are active without much outward movement. Further, 'static load level' referring to the 10th percentile of the APDF, is not task-specific. A misapplication of Jonsson's (1982) recommendations can occur when static and dynamic are thought to be descriptions of work types, rather than components of the APDF (Ankrum, 2000). The miscomprehension of the nomenclature can then lead to job elements being diagnosed as exceeding proposed physical threshold limits when they are actually below them. Although Ankrum (2000) cites several research papers as having misused the static load level proposed by Jonsson (1982), it should be noted that others recognized and accounted for this aspect (Wells et al., 1994).

The guidelines proposed by Jonsson (1982) were established for the shoulder musculature. Similar guidelines are yet to be established for other musculature. This is of some significance as differing muscles and muscle groups have varying numbers of muscle fibers, fiber types, length and relative innervation. The various physical properties of each muscle may

ultimately result in differing times to fatigue. This may negate or require some change in the application of Jonsson's (1982) quantitative threshold values to other muscles.

2.3.6 Hand Activity Threshold Limit Value (TLV) in EDS

Repetitious movements of the hand and wrist during industrial tasks is known to be an important risk factor associated with cumulative trauma disorders (CTDs) (Kvarnstrom 1983; Habes, Carlson & Badger, 1985; Armstrong 1986; Silverstein et al. 1987; Marras 1993). Further, when repetition is combined with forceful work and continued for extended periods, the abilities of individuals to perform these activities are frequently exceeded resulting in severe and chronic injuries (Mital et al. 1993). The ACGIH proposed threshold limit value (TLV) for occupational hand activity levels was developed with expert consensus on the most comprehensive research, guidelines, standards and regulations worldwide. Further, comparative analysis were completed, pitting the TLV against other applicable tools (Moore & Garg, 1995; Snook et al., 1995, 1997). Results purport that use of the TLV will result in less type 1 and type 2 errors. This indicates that in relation to other ergonomic assessment strategies, this tool may be used with greater confidence of worker protection without sacrificing resources to resolve false positive or false negative issues.

In the development of the TLV for hand activity (2001), the ACGIH has plotted normalized peak hand force (NPF), on a scale of 0 to 10, which corresponds to 0 to 100% of the applicable population reference strength. NPF represents the 90th percentile force value so that force would not be driven by random or 'spurious' work elements. The ACGIH (2001) stipulate that for the protection of the worker, the average normalized force should not be greater than 14% of the individuals maximal voluntary contraction (MVC). The normalized force once determined is to be plotted against hand activity level (frequency of hand movements per unit time). The NPF/HAL value would then be compared to the TLV. This ratio is said to provide a threshold limit value that would be applicable to the majority of the working population when applied to cyclical tasks occurring for a duration of no less than 4 hours. The result of this integration is an

inverse linear relationship where force increases and frequency decreases and vice-versa. Force normalization occurs as the analyst adjusts the value obtained to the given population norms (i.e. male mean power grasp value). Further, it is up to the analyst to determine all scaling factors which may alter the strength capability of the individual (i.e. glove use, awkward postures, weak grip, viscosity of object etc.). By using this structure the tool becomes more flexible and may be used across many occupational applications.

2.3.6.1 Limitations of the Hand Activity TLV

The first and most striking limitation of this tool is its lack of field-testing. It is assumed by the developers that the normalized peak force and hand activity aspects of the TLV can be repeatedly obtained between observers through a variety of means. Potvin et al. (2002a) identified the need for comprehensive field-testing and sought to determine the between-rater reliability and the validity of the tool. The validity of the TLV for predicting injuries and discomfort was evaluated using injury data collected from 40 jobs at one plant and from pain and discomfort data across all 280 jobs. Results indicate good between-rater reliability with correlations of more than $r = 0.8$. It was concluded that the TLV guideline can be used by observers for quantifying risk, but decisions regarding the acceptability of a task can only be made with confidence if the TLV risk scores are above +1 or -1.

Ljuggren (1986) and later the ACGIH (2001) reported that it is not necessary to have the individual rate their own perceived exertion, rather this exertion can be estimated by an observer. According to the research of Potvin et al. (2002a), this would in fact be preferable as findings indicate that observers more accurately predict effort values than subjects. In an alternative study by Potvin et al. (2002b), elements of the ACGIH TLV were derived from live observations and from video footage of the same. These were then compared in order to determine the differences if any. The ACGIH (2001) deemed video footage a valid source to obtain values for input into the TLV tool. This study was also designed to quantify the possible differences in scores from external observers and those completing the tasks. Finally, ratings of perceived exertions were

collected to determine which part of the forearm/wrist/hand was most closely correlated with the ultimate peak effort scores obtained from the subjects (Potvin et al., 2002). It was concluded from this study that video recordings were not the best means of obtaining NPF scores and that live observations are preferable. There was however good agreement for HAL between live and video recordings (Potvin et al., 2002).

In summary, the two studies of Potvin et al. (2002a&b) indicate that between-rater reliability is strong, meaning several trained observers are likely to obtain a similar score while observing the same job. Further, observers of a job seem to be better predictors for both HAL and NPF as subjects tended to overestimate by an average of one unit for each (0-10 scale). Validity of the TLV is indicated but using EMG to obtain the NPF and observer ratings for HAL has been suggested as a best practice. Also, if the results fall within a TLV risk score of +/- 1 further investigation is warranted. Finally, it is suggested that the TLV elements be collected from live observations rather than video recordings.

The ACGIH (2001) does not provide any form of weighting or indicated preference in the methods it proposes to collect the NPF aspect of the TLV. Evidently, EMG and observer ratings should be proposed as the primary methods to be used to collect this data. Further, video recordings were used in the beta trials of the tool. This has been shown to be an ineffective means of rating the NPF aspect of the TLV. The ACGIH (2001) may wish to consider retesting with live observations and correlating results to identify anomalies if any.

2.4 Literature Review Summary

This thesis is based on two premises, firstly that there is a positive relationship between work-related musculoskeletal disorders and workplace risk factors. Secondly, that an effective ergonomic process can reduce the potential for the resulting injuries and illnesses by preempting these risk factors. An integral component of this process is a definitive threshold for ergonomic acceptability. As discussed above, several ergonomic tools, aids and guidelines have been refined

and accepted as having thresholds of sufficient sensitivity and specificity to be included within the required tool-set.

The intent of this literature review was to provide evidence of the face validity of the aforementioned ergonomic tools, aids and guidelines. In doing so a summary of the rationale for tool selection, including the development background, assumptions and limitations was necessary. The data gleaned from this was then used as the impetus for the progressive structure of the EDS. This essentially comprises the various levels of questions which are designed to lead the user toward the most appropriate resource during the analysis of a given task. It is the hypothesis of this thesis that both expert and novice subjects, trained in the use of the ergonomic decision system, will reliably arrive at the same decision with regard to the appropriate ergonomic tool while observing the same operation under the same constraints. With that said, the next step requires that the reliability of the decision system be established. This will be accomplished through the review of 6 operations derived from two different facilities by 12 evaluators (6 novice and 6 expert). Details of the strategy are discussed in detail within the following methodology section.

Chapter III METHODOLOGY

3.1 Jobs and Job Selection Criteria

Several Jobs were chosen from two local assembly facilities (Wayne (2), Michigan, USA). One of these facilities manufactures small cars, the other manufactures large sport-utility-vehicles. Facility selection rationale was based on the differing component size, weights and vehicle body spatial elements. These differences may prompt varying selection choices by the subjects and will provide some variety to the sample Jobs.

The Jobs chosen for analysis at each of these facilities were not randomly selected. A large sample of injury and illness data was collected via Incident Investigation Reports of the year 2004. These data were reviewed and filtered for ergonomic implications. These implications, as input by a registered nurse or physician, must have included the terms, "repetitive motion, injury or illness" entered within the "Injury/Illness Type" category of the Incident Investigation Report. Further, in the aforementioned report, under the field of "Incident Analysis, Type of Contact", the category of "Overexertion – Repetitive" must have been entered in order to be included in the study data compilation.

Once refined, the sample list, which resulted in at least one report of occupational injury or illness, included 63 Jobs from the small car assembly plant and 52 Jobs from the large vehicle assembler. These data were then sorted by plant and by severity of incident. Severity was determined by the resulting number of "Restricted Working Days" and number of "Days Away". The number of "Restricted Working Days" indicates that the operator should not be assigned to a task that taxes the body part for which the operator went to Medical. The length of time that an operator is on restricted duty is established by the plant physician. The number of "Days Away" refers to the amount of time that an operator is not available for work due to the medical condition. This decision is also made by the plant physician. Finally, the refined data was reviewed for repeat visits to Medical. This was sorted by "Process Code", which is a systematic

means for the plant to identify a particular operation. If process codes were found to repeat within the filtered database, the Job that they represent was given added weighting in the selection process. Not surprisingly, many Jobs resulting in high-severity medical visits were among those that repeated.

Table 1: Details regarding Restricted Working Days and Days Away for Jobs included in the study

Operation	Restricted Days	Days Away	No. Repeat visits
C40090	13	10	11
T10060	41	12	6
C10130	21	41	4
T60111	26	12	5
TD075L	18	10	6
TE083R	15	11	3

A total of six Jobs were chosen for inclusion in the study, from the two automotive assembly facilities (Table 1). Although each of the Jobs contained many different risk factors, four of the six were selected in order to assess a predominant action (lift/lower etc.) or posture (working overhead etc.). The remaining two represented variations of one of the original four actions and postures. For example, if lifting was to be assessed as one of the predominant actions, two further variations would be presented. Variations may include differences in component weight, size or orientation of the part. The rationale for duplicating an action or posture, with variations, was to provide the subject with a variety of the conditions which may require analysis within an assembly facility, and to assess the decision process under these differing conditions. The Jobs were videotaped from a variety of angles, to provide maximum detail while minimizing the variability which may occur from onsite versus videotape observation (Ericson et al., 1991).

3.2 Subjects

Twelve subjects were chosen to take part in this study. The subjects were divided into two categories. Six of the twelve were expert ergonomic practitioners, with the remaining six having minimal experience in the area of ergonomics. Those deemed as “experts” were required to be

eligible for certification by the Board of Certification in Professional Ergonomics (BCPE). The certification process of the BCPE is a structured approach which evaluates an individual's compliance to technical standards and professional competence in the field of ergonomics (BCPE, 1999). The "novice" subjects were required to have minimal, if any, exposure/experience in the field of ergonomics. This was tested through the application of a 10 question survey. The survey was used relatively simple questions with regard to the basics of ergonomics and task assessment (Appendix B). The individual needed to score less than 5 of 10 correct in order to be rated a Novice.

3.3 Subject Training

Both groups received training in the use of the EDS software. This training of the experts lasted approximately 20 minutes. The training of the novice group lasted approximately 90 minutes. As the training time indicates, the training content differed between the expert and novice groups.

The training of the novice group consisted of many topics including; commonly used term definition, the rationale for an ergonomics process and an introduction to seven ergonomic risk factors with specific examples. Also, novices were provided a detailed review of the systematic ergonomic analysis process and the application, assumptions and limitations of the ergonomic tools that may be used during the process. Finally, the novice group was provided with the same EDS strategy and software training as the experts.

3.4 Data Collection Protocol

Videotaped Jobs were presented to the analysts on a 21" monitor. The EDS software was available on a separate laptop placed adjacent to the viewing monitor. The Jobs were watched in isolation from the other subjects. The 6 Jobs were presented in a random order. The analysts were allowed to take up to 20 minutes to review and enter information for each Job. A 15 minute break was provided at the end of each hour. Analysts had the ability to pause, stop, rewind and play again any Job or Job segment as often as they wished. Each were provided with a pen, blank paper, the user manual for the software and a data sheet containing all pertinent weight, force,

dimensional, and time-related information. Other information requests could be made of the test administrator, who was in the room at all times.

Each Job required decisions at three different levels in the EDS software. The analysts were instructed to inform the test administrator at the time of completion of each of the three Levels. At that time, the analysts were provided with the correct answers for the level, requested to revise their decisions where necessary and instructed to continue to the next Level. As previously mentioned, the EDS was designed on the “minimum spanning tree” concept, in which all relevant information is requested, avoiding erroneous information or duplication. The term “Levels” refers to the gradual refinement of information requests (decisions), until the most applicable ergonomic tool or threshold value is obtained. For example, the initial Level consisted of the decision regarding which actions to include within the Job analysis (push/pull, lift/lower, carry, hand-intensive work). Subsequent levels included decisions regarding the number of hands required to complete the action, the frequency of application, spatial characteristics (grip width etc.), among others (Appendix C). Each decision establishes (effectively eliminates) subsequent choices, until the final and most appropriate tool or final analysis result is realized.

All computer data entry was continuously recorded using HyperCam[®] software and saved to the hard drive. In addition, the results from each subject’s EDS data analysis was saved to the hard drive of the computer upon completion.

Prior to administering the training, novice subjects were presented, and asked to analyze, a randomly chosen Job (Job 1). The training was then provided. Following this, all six Jobs were analyzed by all subjects.

After a two week time period had elapsed after the original analysis, each Expert and Novice subject reanalyzed a Job, randomly chosen from the original six (Job 2). This was designed to assess intra-rater reliability.

3.5 Data Analysis

A criterion measure was necessary in order to determine the accuracy of decision making for each Job/Level combination. The comparative measure or 'gold-standard' was provided through group consensus of three experienced ergonomists, who were identified as having a more intimate knowledge of the EDS process, content and software. Subject responses were considered to be accurate if they matched the consensus of the three experienced ergonomists.

3.5.1 Statistical Analysis

For each Job/Level combination, the decisions made by each subject, were compared with the aforementioned criterion measure. A value of one was assigned to results that matched this criterion measure, while a value of zero was assigned where the subject's selection did not agree with the criterion measure. The results were totaled and averaged across all Jobs and Levels and this value was the total mean consensus for the study. Between subject reliability was calculated by establishing the total average consensus across subjects, using the methods below.

A consensus count, and total mean consensus *between* the 12 subjects, was reviewed for each of the 6 Jobs. The total count was divided by the maximum count (12 for between subjects) to get a percentage of subjects who did or did not concur. The total count was then subtracted from 12 and divided by 12, to determine the percentage of subjects not concurring with the criterion. The higher of the two percentages, was then taken as the percent consensus for each job and level across the twelve subjects. The percentage were then be reduced by 50 and multiplied by 2 in order to get a percent consensus of 0, 33.3, 66.6 or 100 for each level and job. A total mean percent consensus by novice, expert and overall was taken by averaging the total counts (6 jobs by 3 levels). For example, if 4 of 6 expert subjects agreed with the criterion for a Job, the steps would be;

1. $6 - 4 = 2$
2. $2 / 6 = 0.33$ and $4 / 6 = 0.67$
3. Choose 0.67 (larger of 0.33 vs 0.67)
4. $(0.67 - 0.5) * 2 = 0.33$
5. Sum and Average across all Jobs

A 2 x 3 x 6 mixed analysis of variance (ANOVA) was used to evaluate the effects of Experience (expert vs. novice) and their respective decision accuracy over multiple decision Levels (3) across several (6) Jobs (Figure 1). The significance level for each ANOVA was set to $p < 0.05$. The dependent variable is the quantity of errors across Levels and Jobs. For the main effects and interactions, a post hoc analysis was performed using Tukey's honestly significant difference (HSD) ($p < 0.05$). Having rejected the null hypothesis, this test establishes a ratio (effectively a confidence interval) of the difference between two sample means.

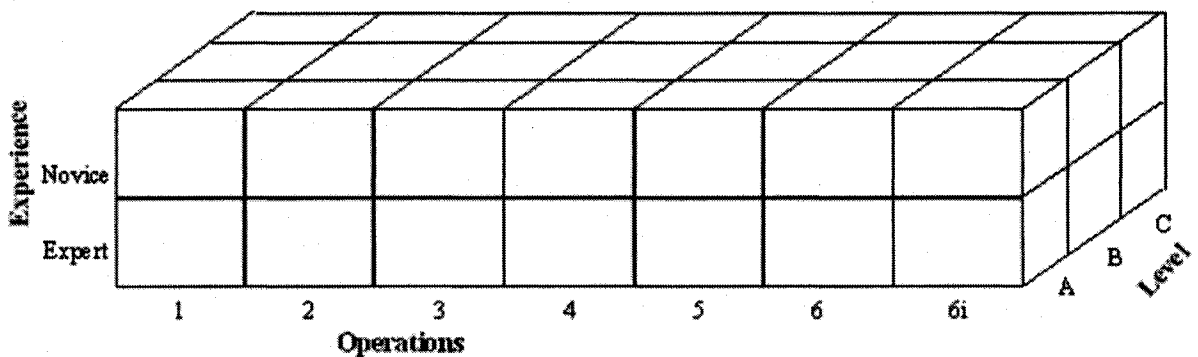


Figure 1: Statistical model for independent variables 1) Jobs, 2) Experience and 3) Level.

Also, a consensus count and total mean consensus count was taken *within* each subject, across these trials for each subject. The total consensus score for each subject and level was averaged. These scores was subtracted from 2 and divided by 2 to determine the number of occurrences where subjects did not concur. The higher of the two results were tabulated. The tabulated values were then reduced in half and multiplied by 2 in order to establish percent consensus. A total mean percent consensus by novice, expert and overall was taken by averaging the total counts (2 jobs by 3 levels). Finally, a consensus count and total mean consensus count, as described above, was used to determine consistency across novice subjects for the pre-training and post training trials.

Chapter IV RESULTS

No data were missing from this collection. Thus, results are reported for all 6 Expert and 6 Novice (n = 12) subjects. The total number of observations was 216 (12 Subjects x 3 Levels x 6 Jobs). The tributary studies of test-retest and of training effects constituted 72 observations (12 Subjects x 3 Levels x 1 Job twice) and 36 observations (6 novice Subjects x 3 Levels x 1 Job x 2 repeats), respectively.

4.1 Between-Subject Reliability

A consensus score was calculated across experts, across novices and across all subjects for each Job/Level combination. The consensus scores ranged from 0% to 100% (Table 2). The overall mean consensus scores are averages across the 12 subjects, not averages between expert and novice means. The averages were: Experts (85%), Novices (72%) and Overall (77%).

Table 2: Mean percent consensus score across all subjects (N = 12).

		Mean		
		Expert	Novice	Overall
Job 1	L1	33%	100%	67%
	L2	100%	100%	100%
	L3	67%	33%	50%
Job 2	L1	100%	67%	83%
	L2	33%	33%	0%
	L3	100%	100%	100%
Job 3	L1	67%	100%	83%
	L2	67%	0%	33%
	L3	100%	100%	100%
Job 4	L1	100%	67%	83%
	L2	100%	67%	83%
	L3	100%	100%	100%
Job 5	L1	67%	33%	50%
	L2	100%	67%	83%
	L3	100%	33%	67%
Job 6	L1	100%	100%	100%
	L2	100%	100%	100%
	L3	100%	100%	100%
Mean		85%	72%	77%

Further, the mean percent consensus was also calculated while pooling by Job (Table 3) and pooling by Level (Table 4).

Table 3: Mean percent consensus score across all subjects pooled by Job.

Pooled by Job	Mean			StDev		
	Expert	Novice	Overall	Expert	Novice	Overall
Job 1	67%	78%	72%	33%	38%	25%
Job 2	78%	67%	61%	38%	33%	54%
Job 3	78%	67%	72%	19%	58%	35%
Job 4	100%	78%	89%	0%	19%	10%
Job 5	89%	44%	67%	19%	19%	17%
Job 6	100%	100%	100%	0%	0%	0%

Table 4: Mean percent consensus score across all subjects pooled by Level.

Pooled by Level	Mean			StDev		
	Expert	Novice	Overall	Expert	Novice	Overall
Level 1	78%	78%	78%	27%	27%	17%
Level 2	83%	61%	67%	28%	39%	41%
Level 3	94%	78%	86%	14%	34%	22%

The mean percent consensus scores ranged from 61% (Job 2) to 100% (Job 6), when pooled for each Job, and from 67% (Level 2) to 86% (Level 3) when pooled for each Level.

4.2 Within-Subjects Reliability

The mean percent consensus for an initial test, and retest two weeks later, was recorded for each subject, across a randomly chosen Job (2) at all 3 Levels. For Job 2, across the six experts and 3 Levels, there were 16 of 18 cases (88.9%) where the first assessment agreed with the second. For the novice subjects, there was 100% consensus from one assessment to the other.

4.3 Within-Subjects Training Effect

A mean percent consensus was taken for each of the novice subjects, across a randomly chosen Job (1) and all 3 Levels, which compared scoring from the pre and post trained subject conditions. There was an 88.9% consensus as 16 of the 18 values agreed pre and post training.

4.4 EDS Utilization Assessment

A mixed analysis of variance was run to determine the main and interaction effects of Experience (between variable), Job and Level (within variables) and the accuracy of EDS utilization (Table 5). All data are summarized in Table 6.

Table 5: ANOVA table for the main and interaction effects of Experience, Job and Level on accuracy of FEDs utilization.

ANOVA Table for Score

	DF	Sum of Squares	Mean Square	F-Value	P-Value	Lambda	Power
Experience	1	.375	.375	2.238	.1656	2.238	.262
Subject(Group)	10	1.676	.168				
Task	5	.968	.194	3.719	.0061	18.594	.910
Task * Experience	5	.486	.097	1.868	.1167	9.342	.583
Task * Subject(Group)	50	2.602	.052				
Level	2	.343	.171	1.745	.2002	3.491	.312
Level * Experience	2	.250	.125	1.274	.3016	2.547	.236
Level * Subject(Group)	20	1.963	.098				
Task * Level	10	2.713	.271	2.733	.0052	27.332	.960
Task * Level * Experience	10	.806	.081	.812	.6181	8.116	.399
Task * Level * Subject(Group)	100	9.926	.099				

Table 6: Individual results and means across Experience, Job and Level.

		Job 1			Job 2			Job 3			Job 4			Job 5			Job 6			Mean	
		L1	L2	L3	L1	L2	L3	L1	L2	L3	L1	L2	L3	L1	L2	L3	L1	L2	L3		
Expert	E1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	100%	
	E2	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	100%	
	E3	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	100%	
	E4	0	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1	94%	
	E5	0	1	1	1	0	1	0	1	1	1	1	0	1	1	1	1	1	1	78%	
	E6	1	1	0	1	0	1	1	0	1	1	1	1	1	1	1	1	1	1	83%	
Novice	N1	1	1	1	1	0	1	1	1	1	1	1	0	1	1	1	1	1	1	89%	
	N2	1	1	1	1	1	1	1	0	1	1	1	1	1	0	1	1	1	1	89%	
	N3	1	1	0	0	0	1	1	0	1	0	1	1	1	0	1	1	1	1	67%	
	N4	1	1	0	1	0	1	1	0	1	1	1	1	1	1	1	1	1	1	83%	
	N5	1	1	1	1	0	1	1	1	1	0	1	1	1	0	1	1	1	1	83%	
	N6	1	1	1	1	1	1	1	1	1	1	1	1	0	1	1	1	1	1	94%	
Mean by Job	86.1%			80.6%			86.1%			94.4%			83.3%			100.0%			88.4%		
Mean by Level	L1	L2	L3																		
		88.9%	83.3%	93.1%																	

4.4.1 Experience Effect

The ANOVA indicated that Experience did not have a significant main or interaction effect on accuracy (Table 5). However, the average accuracy of the expert (92.6%) had a tendency to be 8.3% better than that of the novice (84.3%) (Table 6).

4.4.2 Job Effect

The within subject variable of Job demonstrated the only significant main effect ($p = 0.0061$) (Table 5). The accuracy scores ranged from 80.6% (Job 2) to 100% (Job 6) with an overall mean of 88.4% (Table 6). Significant interactions were found between Jobs x Levels. As such post hoc values will be reviewed in light of the interaction.

4.4.3 Level Effect

There was no significant main effect of the within subject variable of Level on the accuracy scores (Table 5). The range of scores across levels ranged from 83.3% (Level 2) to 93.1% (Level 3) (Table 6).

4.4.4 Job & Level

There was a significant Task x Level interaction ($p = 0.0052$) (Table 5, Figure 2). The means of the individual Levels were compared within each Job. For Job 2, Level 2 was significantly different from both Level 1 ($p \leq 0.05$) and Level 3 ($p \leq 0.05$). For Job 3, Level 2 was significantly different from Level 3 ($p \leq 0.05$).

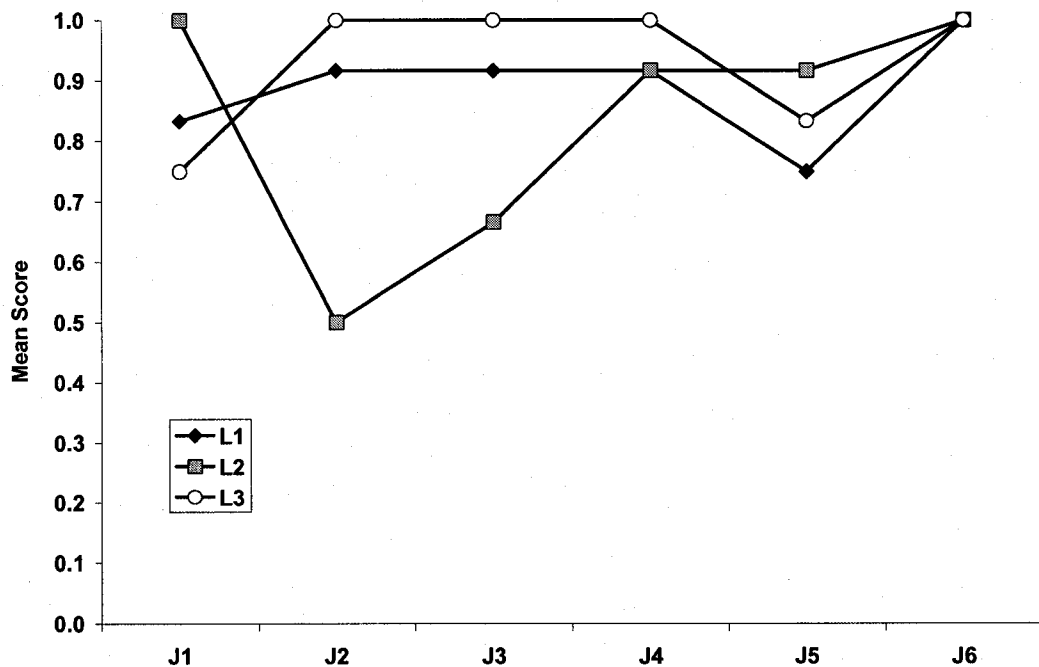


Figure 2: Total mean score for all subjects ($n = 12$) by Job x Level interaction.

Chapter V

DISCUSSION

The purpose of this thesis was to establish the reliability and face validity of a unique ergonomic process, deemed the Ergonomic Decision System. The rationale for the development of the EDS was due to a clear lack of existing reliable, accurate and timely analysis strategies (Brodie & Wells, 1997). Face validity was established via an in-depth literature review, from which the content of the decision system was developed. The between and within-rater reliability of the decision system were established from controlled testing with a number of trained ergonomic engineers and novices working in isolation, under time constraints and using the process in an attempt to analyze several jobs. Particularly, this study was designed to determine if the EDS is reliable across individuals (both expert and novice) and meets established time requirements such that it can be shown to be a relatively non-invasive and comprehensive tool.

For an ergonomic system to be useful, the elements within must provide a reliable, accurate measure of the desired variable. Accurate and consistent values provide confidence for the predictive ability of the system (Brodie & Wells, 1997). For the purpose of this study, accuracy was defined as concurrence with the criterion measure. Consensus scores were used to gauge reliability between and within subjects, while raw scores were used to provide accuracy values.

5.1 Subject Accuracy

The overall mean concurrence with the criterion measure was an impressive 88.4%, with experts scoring 92.6% and novices 84.3%. When scrutinized more closely, it can be seen that experts tended to score better than novices on 4 out of 6 Jobs. When individual scores were reviewed, the range for all 6 novice subjects was 67% (subject 3) to 94% (subject 6) and for experts was 78% (subject 5) to 100% (subjects 1,2,3).

The congruency of the results was particularly impressive, given the limited ergonomic skill level of the novice subjects, as evidenced by their ergonomic survey scores (mean 17%) and

the minimal training provided. The data indicate that experience should only minimally impact accuracy, with results of the study providing statistical confirmation that experts and novices achieved high accuracy and differ insignificantly in their concurrence with the criterion metric for correct responses.

Mean accuracy scores for individual Jobs ranged from 81% (Job 2) to 100% (Job 6). Though the data indicates that both novice and expert subjects had the lowest accuracy on Job 2, the largest discrepancy was shown between the two groups on Job 5, with an average score of 72.2% for novices and 94.4% for experts. Job 5 (wire route and secure) required significant identification of many fine motor movements, as it contained wire manipulation and six electrical connections. Fine motor movements are difficult to assess, as they are generally difficult to see from video and are often poorly identified (Brodie & Wells, 1997). It would seem that the inaccuracy in novice scoring on Job 5 may be attributable jointly to inexperience in the field (Tolmie, 2002) and to inherent difficulties with observing operations through the medium of video recordings (Grieve et al., 1975). Some of these difficulties include the identification of joint angles, temporal aspects and force estimations which, due to their lack of experience, novice subjects may not be as able to identify from video footage.

The average accuracy was 88.9%, 83.3% and 93.1% for Levels 1, 2 and 3 respectively. Task x Level demonstrated the only significant interaction for accuracy. Post hoc analysis of this interaction indicated that that Level 2 was significantly different than: 1) both Levels 1 and 3 for Job 2 and 2) Level 3 for Job 3. Specifically, certain elements contained within Level 2 of both Jobs 2 and 3 tended to result in inaccurate results. For Job 2 (alternator build-up/ install), the Level 1 gross motor element of lifting was identified well with 92% accuracy (100% expert, 83% novice) however, the modification of this element required at Level 2 presented difficulty with 50% accuracy (67% expert, 33% novice). Specifically, the differentiation of 1 hand versus 2 for the lift posed a problem for all subjects. For Job 3 (12A581 wire harness install), the Level 1 element of 'awkward posture' was again identified well with 92% accuracy (83% expert, 100%

novice) however, for Level 2 this score was reduced to 67% (83% expert, 50% novice). In particular, the Level 2 element requiring differentiation between holding the posture cumulatively for less than or greater than 50% of the cycle time presented the most difficulty, especially for the novice group. The rationale for this seemingly reduced ability to accurately identify the Level 2 elements may be attributed to the fact that it requires modification of the initial, gross action/posture identification into more refined posture, frequency and spatial characteristics (Brodie and Wells, 1997). It would seem that all subjects have difficulty with this, specifically novice subjects seem to find the refinement most problematic. The details of these difficulties will be discussed further in the next section.

5.2 Subject Consistency

Subject consistency was evaluated by consensus scoring. The mean overall consensus, between subjects, was 76.9%, across all 6 Jobs x 3 Levels. The mean consensus for experts was 85% and for the novice group was 72%. These figures were scrutinized by Job x Level in order to identify and discuss the significant findings (Figure 3).

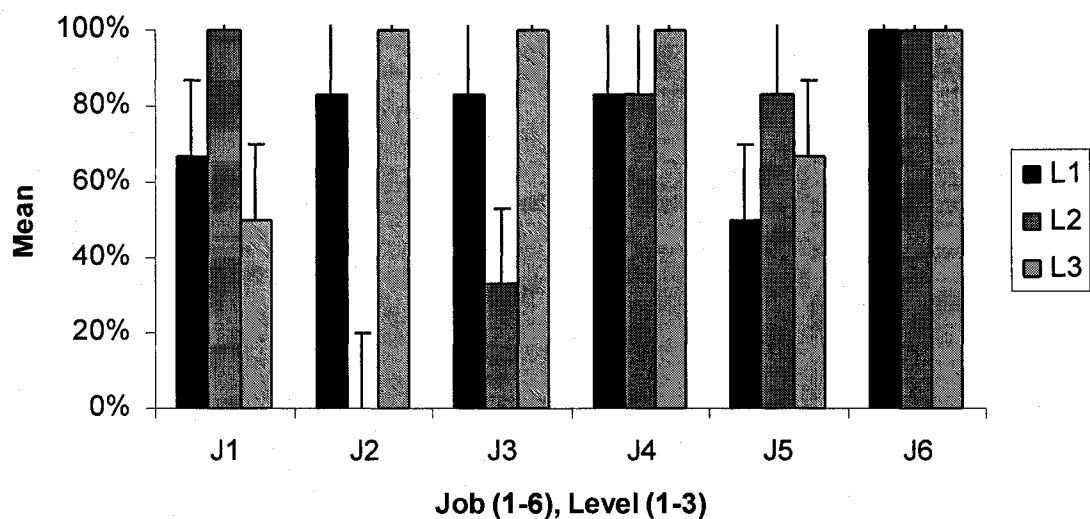


Figure 3: Total mean consensus score for all subjects (n = 12) by Job x Level interaction.

The mean consensus score, pooled within Jobs, ranged from 61% (Job 2) to 100% (Job 6). Reviewing this in detail, all subjects showed perfect consistency on Job 6 (power steering and

transmission line secure) across all Levels. This Job was unique in that, unlike the other five Jobs which focused mainly on rapid and repeated movements, the main element of this Job was a posture, specifically, conducting work with the hands overhead. From the video, it was very evident that this was the case. Consequently, none of the subjects missed this gross movement and posture (Brodie & Wells, 1997). Further, since all of the work in Job 6 was overhead, identifying the time overhead was not difficult. Also, subjects were more vocal in questioning the test administrator for this operation, which may have led to correct answers. Finally, this was the final Job that the subjects were presented, as such learning may have occurred. It should be noted that subjects achieved perfect consensus on Level 3 across four of the six Jobs. This may have been a result of Level 3's content. Typical requirements of Level 3 are the identification of direction or time elements. The direction of vertical, lateral or horizontal movements are reasonably apparent for gross motor movements (Eastman Kodak, 1986). Time may have been obtained from the video footage itself or by requesting the specific answer from the test administrator.

The overall consensus averages for Levels 1, 2, 3 were 77.8%, 66.7% and 86.1%, respectively. When the interactions are reviewed, the consensus scoring on Level 2, versus that of 1 or 3, was substantially lower less than the overall average (76.9%) for both Jobs 2 (0.0%) and 3 (33.3%). The rationale for this seemingly reduced ability to consistently identify the Level 2 elements may be attributed to the fact that it requires modification of the initial Level elements by posture, frequency and spatial characteristics. For example, if the subject identified the Level 1 element of lifting, the Level 2 would require the subject to identify the number of hands used, whether the horizontal distance from the body to the coupling point (hands) is less than 19", whether the vertical span of the hands are less than 26" and the number of objects lifted per cycle. Thus, as supported by the findings of Brodie and Wells (1997), the Level 1 choice of the initial gross action tended to be identified very effectively. Whereas, movements that were hard to

define (temporal elements, rapid movements), postures of smaller joints (elbow, wrist) and items that were hard to see from video (mass, force), were more difficult to identify.

Though the observer had the ability to rewind and review the operation freely, and to ask pertinent questions of the independent observer, certain aspects may not have been easily identifiable from the video footage, or a visual cue may have been missed. In fact, when the data associated with Job 2/Level 2 is scrutinized, 80% of the total error can be attributed to a missed identification of a one-handed lift. This miss may have been caused by some confusion related to whether the operator *needed* to lift the object with one-hand, or whether the operator *choose* to lift the object with one-hand. If the latter was the case, a subject may have ignored the one-handed aspect, in favor of selecting of a two-handed lift.

Job 3/Level 2 was also observed to have a low consensus score (33%). When the errors were reviewed, it was identified that, in all cases, the differences were due to the misinterpretation of the amount of time that an individual sustained a posture. The error code was documented as, "*awkward posture held greater than 50% of the cycle time*" where the correct answer was less than 50%. According to the studies of both Brodie and Wells (1997) and Grieve et al. (1975), the temporal aspect of the operations would be classified as an element that was hard to quantify from video. It should, however, again be noted that the observer was free to review the operation until comfortable with their response and could ask pertinent questions at any time. With this said, technological error, or error with the measurement system, should not be implicated in the failure of the observer to attune themselves to this element. Further, human elements such as subject motivation or attention, may have contributed to these errors (Spatz & Johnston, 1989).

Clearly there were certain Levels within Jobs that had lower consensus than others, with a range from 0.0% to 100%. However, Fleiss' kappa coefficient for agreement (1986) stipulates the overlay of mean agreement scores to particular categories ranging from excellent agreement (> 0.75), to fair/good agreement ($0.4 - 0.75$) to poor agreement (< 0.4). Adapting the current

study results to these scales, with the overall between rater consensus levels at 76.9%, and a minimal span between expert and novice (85.2% vs. 72.2% respectively), it may be stated that all subjects were capable of consistently cuing to and identifying the required elements of the decision system.

5.2.1 Test-Retest Reliability

Overall, subjects demonstrated good consensus for the test-retest condition (94.4%). The average consensus for experts was 88.9%, where novice subjects showed perfect consensus. This would indicate that the experimental design was reliable and consistent, such that limited differences in responses would be expected regardless of time of testing.

While reviewing the consensus data, it is evident that, although a minimum of two weeks had passed since the primary testing, the two experts, who did not concur with the criterion measure for the first trial, corrected themselves for the second. The four novice subjects, who did not concur with the criterion value for the first trial, did not do so again for the second. It appears that experience is an important factor in variation and that, although the novice subjects did have substantial training, they were attending to (or missing) the same cues trial after trial where the experts learned from the previous mistake and attended to novel cues on the next opportunity.

The statistical analysis indicated that there was limited change between the means in the test and retest trials. As mentioned previously, the same four novice subjects consistently failed to concur with the criterion measure on the same Level (2) throughout the test and retest. This would indicate that the study protocol was effectively designed to provide consistent results over time. The testing made use of controlled verbiage and presented the same information to each individual in the same manner each and every time. The operations were presented to each subject in the same manner, as they were recorded and reviewed on a video monitor in a controlled environment. With all input elements fixed, the results would lead to the conclusion that the study protocol and the EDS allowed subjects to perform consistent analyses.

5.2.2 Training Effect

A study was conducted to determine the effect of training on novice subjects. As with the above test-retest condition, a strong consensus was found in the responses before and after training, with an average of 88.9%. The novice subjects all had to take a screening test prior to taking part in the study. The results of the test (Appendix B) indicated that the initial ergonomic skill set was minimal with an average score of 17%. The results would seemingly indicate that the ergonomic decision system is intuitive and reasonably easy to use and understand across skill levels, even in the absence of significant training.

5.3 EDS Limitations

The choice of Job 1 for the training effect study was done randomly. Pre training-post training data indicate that scores within and between operators for Job 1 had good consensus (72%) and accuracy scores approaching the mean value (86.1%). By chance, another Job could have been chosen for this scenario. Based on the post-trained data, one may anticipate that if the randomly chosen job were, for example Job 2 or 5, the scores on the initial, pre-trained condition may have resulted in a substantially worse outcome. Assuming that the training had some effect, the post-trained accuracy may have increased, and consensus may have changed to some extent. One must therefore question whether the effectiveness of the training was truly tested or whether the randomly chosen Job and its Levels were intuitive.

The choice of operation for the within-subject reliability study was also done randomly. The selected Job (2) had very high consensus scores across the two trials, with novice subjects scoring with low accuracy (33%), but perfect consensus. The test-retest took place after the subjects were trained, therefore one would have to question whether some element in the training lead to the repeated and consistent errors in novice subjects.

The subjects themselves may have induced some randomness into the study. For instance, each novice subject received the same ergonomics training, and each expert and novice received the same training in the use of the EDS. It is not possible, however, to determine the

retention of information that had occurred or whether the subjects could truly apply it. Further, the motivation of the subject may have positively or negatively impacted the subjects score on each task. One may use time-to-complete as a surrogate measure of motivation but this is suspect information and should be used cautiously (Eastman Kodak Company, 1986).

The six Jobs in this study were not chosen at random but, rather, were selected based on their having a high incidence of injury, illness and medical data. However, they were chosen from a large pool of jobs with very similar data, and were chosen to represent a number of working conditions representing two facilities with varying dynamics. One of the facilities produced very large vehicles and, consequently, has many very large parts. The other facility produces a very small vehicle and has many small parts. It should be noted, however, that the six Jobs did not cover all elements of Level 1, 2 or 3 of the EDS. Therefore, the current study is limited to the elements included within the Jobs reviewed. Like most research, one would have to make certain assumptions about the applicability of the tool to each unique particular circumstance prior to use.

Video recordings have many desirable features, such as allowing an analyst to review the operation multiple times and being sure that each time the footage is reviewed, it will be exactly the same. However, there are also limitations associated with using video footage. For instance, the ability to assess quantitative values is limited (Tolmie, 2002). For example, all subjects would have difficulty accurately determining a force value while observing an experienced worker horizontally push one component into another (i.e. Job 1, Halfshaft install). These values would have to be quantified and provided to the observer. Further, certain elements have been found to be particularly difficult to determine from video, such as twisting, rapid rotation, contact stress, vibration, and fine movements (Brodie & Wells, 1997). Through this study, it was determined that it is difficult to view certain tasks performed in tight spaces. Also, the ability to communicate with the operator may provide insight into unobserved but difficult elements of the Job, such as retrieving stock or flooring conditions. Video footage should be collected from

multiple positions, angles and distances, with the intent to provide as much detail as possible. This reduces the variability caused by on-site versus videotape analysis (Douwes & Dul, 1991). The video recordings used within this study were taken with one camera, through a variety of angles, in an attempt to adhere to the aforementioned protocol. It should be noted that on-site viewing would present opportunities that this video footage did not. However, if this study had used on-site viewing it would likely have come at a cost of controlled observation. Due to shift scheduling, formal and informal breaks and other factors on site, field observation often results in the viewing of different workers completing the job, often in different ways. This variability would make it difficult to properly assess the decision system.

The Jobs were filmed and digitally recorded. It should be noted however that these Jobs were then presented to each subject in the same order, meaning Job 1 through 6 were common across subjects. Though all subjects achieved perfect consensus and accuracy on Job 6, no linear or curvilinear pattern is evidenced across Jobs or Levels. The results indicate that there is minimal indication of an order effect (Figure 2).

The EDS has been developed, and designed for use, within the automotive industry. Its applications are therefore primarily intended for use within this sector. However, the human body is bound by the balance between tissue demand and tolerance, not by the particular commodity which they assemble. In addition, the Ergonomic tools incorporated into the EDS are not specific to the automotive assembly industry. Therefore, the EDS tool should, theoretically, be applicable to any working environment where the initial actions or postures may take place.

Chapter VI CONCLUSION

This study sought to evaluate the accuracy and reliability of a novel ergonomic decision system. The results indicate that accuracy was very high, with an overall mean of 88%, and consistency data was also very strong with an overall between-user consensus of 77%. With this, the data indicates that users of the EDS produced accurate and reliable results across subjects. The original hypothesis was that both expert and novice subjects, trained on the ergonomic decision system, would consistently arrive at the correct decision with regard to the appropriate ergonomic tool while observing the same operation under the same constraints. When the results of the study were run through an analysis of variance, there were no significant main or interaction effects of experience. However, experts tended to be more accurate at 93% than novices at 84%. The data indicate that the EDS accurately leads novice and expert subjects to arrive at an analysis that agreed with the criterion measure. With this, the purpose was achieved and the hypothesis should be accepted.

It was noted at the onset of this thesis that the EDS would need to be proven capable of meeting the automotive manufacturing industry's requirements. These requirements stipulated that the face validity be established for the ergonomic tools, which are essentially the foundation of the EDS. This was accomplished with a detailed review of literature that outlined the research behind each tool, their individual criteria and their limitations. It was further stipulated that, in order for the EDS to be useful, it must be able to be consistently applied by multiple analysts. Otherwise, the direction of certain costly ergonomic decisions may depend on the EDS user. With the high consistency and accuracy data provided, it can be stated that the EDS has been proven to be reliable between and within individuals, able to be administered within reasonable time constraints, relatively non-invasive and comprehensive.

The EDS is a system intended to allow both experts and novices to systematically break a Job into component elements and progressively arrive at the same and most appropriate

ergonomic tool for analysis. It is not, however, intended to completely analyze an operation. If such an analysis was needed, it would require an individual who is sufficiently trained in the use of the individual tools, and understands the limitations and assumptions of each. This system does not sufficiently arm the user with this knowledge.

6.1 Future Direction

The intent of designing and testing this ergonomic decision system was to disseminate it throughout a major original equipment manufacturer (OEM). This system provides a means to empower many more employees, and to focus limited resources on the most appropriate ergonomic targets, in the hope of abating future injury or illness.

With the implementation of the EDS, a concentrated focus should be given to gathering feedback on its usability, impact on injury statistics. In addition, a comparison should be made with data which would have been used if the tool was not provided. The EDS should also be considered a 'living entity', such-that new and pertinent research should continuously be reviewed and, if deemed to be of sufficient sensitivity and specificity, incorporated into the system.

Further attention should be given to the novice subject training. The results of the data analysis were inconclusive, in that there was little apparent effect of the training. With the current results, it is difficult to determine whether the training had an impact, whether the tool is naturally intuitive or whether it was the job itself that provided evident elements that could easily be attended to. It may be necessary to improve the novice training in order to further reduce errors.

Equal weighting was given to the training of subjects for each of the action and posture categories included within the EDS. Some of these elements require gross movements of large body segments (lifting or working overhead). It would seem that, based on the findings of this study and those previously cited, more focus should be given to the identification and analysis of fine motor tasks versus that of gross. In particular, dedicated training on the video analysis of

hand activity tasks should be added. This finding is an unexpected but important aspect of this study and should be considered for future research.

REFERENCES

- Aaras, A. and Westgaard, R.H. (1987). Further studies of postural load and musculoskeletal injuries of workers at an electro-mechanical assembly plant. *Applied Ergonomics*, 18, 211-219.
- Aaras, A. (1994). Relationship between trapezius load and the incidence of musculoskeletal illness in the neck and shoulder. *International Journal of Industrial Ergonomics*, 14, 341-348.
- Aghazadeh, F. (1998). Models for lifting load capacity of Indonesian population. *Occupational Ergonomics*, 1 (1), 67-74.
- Akella, P. and Peacock, B. (1999). Intelligent Assists: A new generation of ergonomic tool. *Applied Ergonomics, Case Studies*, 2, 91-101.
- American Conference of Governmental Industrial Hygienists (ACGIH)(2001). *Threshold Limit Value: Hand Activity Level*. Cincinnati, OH: American Conference of Governmental Industrial Hygienists.
- Andersson, G.B.J. (1981). Epidemiologic aspects of low-back pain in industry. *Spine*, 5, 245-253.
- Andrews, R.B. (1967). Estimation of values of energy expenditure rate from observed values of heart rate. *Human Factors*, 9 (6), 581-586.
- Ankrum, D. (2000). On the confusion between static load level and static task. *Applied Ergonomics*, 31, 545-546.
- Armstrong, T., Chaffin, D.B. and Foulke, J.A. (1979). A methodology for documenting hand positions and forces during manual work. *Biomechanics*, 12, 131-133.
- Armstrong, T., Foulke, J., Joseph, B. (1982). Investigation of cumulative trauma disorders in a poultry processing plant. *American Industrial Hygiene Association Journal*, 43, 103-115
- Armstrong, T. (1986). Ergonomics and cumulative trauma disorders. *Hand Clinics*, 2 (3), 553-565.
- Armstrong, T., Buckle, P., Fine, L., Hagberg, M., Jonsson, B., Kilbom, A., Kourinka, I., Silverstein, B., Sjogaard, G. and Viikari-Juntjura, E. (1993). A conceptual model for work-related neck and upper-limb musculoskeletal disorders. *Scandinavian Journal of Work. Environment and Health*. 19, 73-84.
- Armstrong, T., Foulke, J., Latko, W., Raybourn, R., Ulin, S. (1996). Work related musculoskeletal disorders of the upper limb: Exposure evaluation. *Advances in Occupational Ergonomics and Safety*, 1, 405-410.
- Armstrong, T. (2002). Analysis of the human-machine system: Identification of anthropometric requirements. Retrieved July 13, 2003, from <http://ioe.engin.umich.edu>

- Astrand, P.O. and Rodahl, K. (1977). Textbook of Work Physiology, second edition. New York, NY. McGraw-Hill Inc.
- Astrand, P.O. and Rodahl, K. (1986). Textbook of Work Physiology, third edition. New York, NY. McGraw-Hill Inc.
- Ayoub, M.M., Gidcumb, C.F., Hafez, H., Intaranont, K., Jiang, B.C. and Selan, J.L. (1983). A Design Guide for Manual Lifting Tasks. Prepared for OSHA. In A Guide to Manual Materials Handling, Mital, A., Nicholson, A.S. and Ayoub, M.M. (1993). Washington, DC. Taylor & Francis Inc.
- Ayoub, M.M. and Mital, A. (1989). Manual Materials Handling. London, UK. Taylor & Francis.
- Board of Certification in Professional Ergonomics (BCPE) (1999). Board of Certification in Professional Ergonomics Candidate Handbook: Certification Policies, Practices and Procedures. Bellingham, WA: Board of Certification in Professional Ergonomics.
- Bink, B. (1962). The physical working capacity in relation to working time and age. *Ergonomics*, 5, 25-28.
- Baidya, K.N. and Stevenson, M.G. (1988). Local muscle fatigue in repetitive work. *Ergonomics*, 31 (2), 227-239.
- Baron, S. (1996). Evaluation of symptom surveys for occupational musculoskeletal disorders. *American Journal of Industrial Medicine*, 29 (6), 609-617.
- Barsky, I. And Dutta, S.P. (1997). Cost assessment for ergonomic risk (CAFER). *International Journal of Industrial Ergonomics*, 20, 307-315.
- Basmajian, J.V. and DeLuca, C.J. (1985). *Muscles Alive – Their functions revealed by electromyography*, fifth edition. Baltimore, MD. Williams & Wilkins.
- Bergmasco, R., Girola, C. and Colombini, D. (1998). Guidelines for designing jobs featuring repetitive tasks. *Ergonomics*, 41 (9), 1364-1383.
- Borg, G.A.V. (1973). Perceived Exertion: A note on history and methods. *Medicine and Science in Sports*, 5 (2), 90-93.
- Borg, G.A.V. (1982). Psychophysical bases of perceived exertion. *Medicine and Science in Sports and Exercise*, 14 (5), 377-381.
- Brodie, D. and Wells, R. (1997). An evaluation of the utility of three ergonomic checklists for predicting health outcomes in a car manufacturing environment. *Proceedings of the 29th Annual Conference of the Human Factors Association of Canada*, 45-52.
- Bureau of Labor Statistics (BLS). (2003). Industry Injury and Illness Data. Summary tables. Retrieved June 28, 2003, from <http://www.stats.bls.gov/iif/oshsum.htm>.
- Burrows, E., Jenkins, S., Thomas, G. and Rickards, J. (1998). A pre-intervention benefit/cost methodology – Refining the cost audit process. *Proceedings of the 30th Annual Conference of the Human Factors Association of Canada*, 131-135.

- Chaffin, D.B. (1967). The development of a prediction model for the metabolic energy expended during arm activities. In Garg, A., Chaffin, D.B. and Herrin, G. (1978). Prediction of metabolic rates for manual materials handling jobs. *American Industrial Hygiene Association Journal*, 39 (8), 661-674.
- Chaffin, D.B. and Park, K.S. (1973). A longitudinal study of low-back pain as associated with occupational weight lifting factors. *American Industrial Hygiene Association Journal*. 32, 513-525.
- Chaffin, D.B., Herrin, G.D. and Keyserling, W.M. (1978). Preemployment strength testing: An updated position. *Journal of occupational medicine*, 20, 403-408.
- Chaffin, D.B. and Andersson, G.B.J. (1991). *Occupational Biomechanics* (2 ed.). New York, NY: John Wiley & Sons, Inc.
- Chaffin D.B. and Erig, M. (1991). Three-dimensional biomechanical static strength prediction model sensitivity to postural and anthropometric inaccuracies. *IIE Transactions*, 23 (2), 215-227.
- Chaffin, D. B., Andersson, G. B. J. & Martin, B. J. (1999). *Occupational Biomechanics* (3 ed.). New York, NY: John Wiley & Sons, Inc.
- Chen, J., Jianwen, C. and Zhou, H. (2004). Two-step estimation for a generalized linear mixed model with auxiliary covariates. *Statistica Sinica*, 14, 361-376.
- Christensen, H. (1986). Muscle activity and fatigue in the shoulder muscles during repetitive work. *European Journal of Applied Physiology*, 54, 596-601.
- Ciriello, V.M. and Snook, S.H. (1983). A study of size, distance, height, and frequency effects on manual handling tasks. *Human Factors*, 25, 541-550.
- Ciriello, V.M., Snook, S.H., Blick, A.C. and Wilkinson, P.L. (1990). The effects of task duration on psychophysically-determined maximum acceptable weights and forces. *Ergonomics*, 33 (2), 187-200.
- Coggon, D., Rose, G. and Barker, D.J.P. (1997). *Epidemiology for the Uninitiated*, Fourth edition. BMJ Publishing Group. On: <http://bmj.bmjournals.com/epidem/epid.html>.
- Damkot, D.K., Pope, M.H., Lord, J. and Frymoyer, J.W. (1984). The relationship between work history, work environment and low back pain in men. *Spine*, 9, 395-399.
- Deal, G. (1995). *Factors Affecting Acceptable Rate of Manual Mating of Connectors*. PhD. [Dissertation], University of South Florida, Tampa, Florida.
- Dempsey, P.G., Sorock, G.S., Cotnam, J.P., Ayoub, M.M., Westfall, P.H., Maynard, W., Fathallah, F. and O'Brien, N. (2000). Field evaluation of the revised NIOSH lifting equation. *Proceedings of the IEA 2000/HFES 2000 Congress*.
- Dennett, X., Fry, H. (1988). Overuse syndrome: A muscle biopsy study. *Lancet*, April, 905-908.

- Department of Labor and Industries (1988). Regulations and Code of Practice: Manual Handling. Victoria: Department of Labor.
- Dolan, P., Adams, M.A. and Hutton, W.C. (1988). Commonly adopted postures and their effect on the lumbar spine. *Spine*, 13 (2), 197-201.
- Douwes, M. and Dul, J. (1991). Validity and reliability of estimating body angles by direct and indirect observations. In *Designing for Everyone*. Queinnec and Daniellou (Eds.). London, Taylor & Francis.
- Dul, J. (1988). A biomechanical model to quantify shoulder load at the work place. *Clinical Biomechanics*, 3, 124-128.
- Eastman Kodak Company (1986). *Ergonomic Design for People at Work, Volume 2*. New York, N.Y.: International Thomson Publishing, Inc.
- Elliott, B. C. and Wood, G. A. (1995). *Science and Sport in Medicine: Biomechanical Principles*. Victoria, Australia: Blackwell Science Pty Ltd.
- Engstrom, T., Hanse, J., Kadefors, R. (1998). Musculoskeletal symptoms due to technical preconditions in long cycle time work in an automobile assembly plant: a study of prevalence and relation to psychosocial factors and physical exposure. *Applied Ergonomics*, 30, 443-453.
- Ericson, M., Kilbom, A., Wiktorin, C. and Winkel, J. (1991). Validity and reliability in the estimation of trunk, arm and neck inclination by observation. In Y. Quéinnec and F. Daniellou (Eds.). *Designing for Everyone*. New York, NY: Taylor & Francis.
- Fernandez, J.E., Ayoub, M.M. and Smith, J.L. (1991). Psychophysical lifting capacity over extended periods. *Ergonomics*, 34 (1), 23-32.
- Feuerstein, M. and Fitzgerald, T. (1992). Biomechanical factors affecting upper extremity cumulative trauma disorders in sign language interpreters. *Journal of Occupational Medicine*, 34 (3), 257-264.
- Fisher, D.L., Andres, R.O., Airth, D. and Smith S.S. (1993). Repetitive Motion Disorders: The Design of Optimal Rate-Rest Profiles. *Human Factors*, 35 (2), 283-304
- Fleiss, J.L. (1986). *The Design and Analysis of Clinical Experiments*. John Wiley & Sons, Toronto.
- Foreman, T.K., Baxter, C.E. and Troup, J.D.G. (1984). Ratings of acceptable load and maximal isometric lifting strengths: the effects of repetition. *Ergonomics*, 27 (12), 1283-1288.
- Frankel, V. H. and Burstein, A. H. (1970). *Orthopaedic Biomechanics*. Philadelphia, PA: Lea and Febiger.
- Frederick, W. (1959). Human energy in manual lifting. *Modern Materials Handling*, 14 (3), 74-76.
- Friedman, G.D. (1974). *Primer in epidemiology*. New York, NY: McGraw-Hill.

- Frymoyer, J.W., Pope, M.H., Costanza, M.C., Rosen, J.C., Goggin, J.E. and Wilder, D.G. (1980). Epidemiologic studies of low-back pain. *Spine*, 5 (5), 419-423. Gamberale, F., Ljungberg, A.S., Annwall, G. and Kilbom, A. (1987). An experimental evaluation of psychophysical criteria for repetitive lifting work. *Applied Ergonomics*, 18 (4), 311-321.
- Garg, A. (1976). A metabolic rate prediction model for manual materials handling jobs. Ph.D Dissertation, University of Michigan.
- Garg, A., Chaffin, D.B. and Herrin, G. (1978). Prediction of metabolic rates for manual materials handling jobs. *American Industrial Hygiene Association Journal*, 39 (8), 661-674.
- Garg, A. and Saxena, U. (1982). Maximum frequency acceptable to female workers for one-handed lifts in the horizontal plane. *Ergonomics*, 25 (9), 839-853.
- Garg, A. (1983). Physiological responses to one-handed lift in the horizontal plane by female workers. *American Industrial Hygiene Association Journal*, 44 (3), 190-200.
- General Accounting Office/ Health Education and Human Services Division (GAO/HEHS)(1997). United States General Accounting Office Report to Congressional Requestors: Worker Protection, Private Sector Ergonomics Programs Yield Positive Results. Washington, DC.
- Giroux, B. & Lamontagne, M. (1992). Net shoulder joint moment and muscular activity during light weight handling at different displacements and frequencies. *Ergonomics*, 35 (4), 385-403.
- Gescheider, G.A. (1997). *Psychophysics, the fundamentals*. Third edition. Mahwah, NJ. Lawrence Erlbaum Associates, Inc.
- Glover, J.R. (1970). Occupational health research and the problem of back pain. *Transactions of the Society of Occupational Medicine*, 21, 2-12.
- Goldstein, S., Armstrong, T., Chaffin, D., Matthews, L. (1987). Analysis of cumulative strain in tendons and tendon sheaths. *Journal of Biomechanics*, 20 (1), 1-6.
- Gravetter, F. and Wallnau, L. (1988). *Statistics for the behavioral sciences*, third edition. New York, NY. West Publishing Co.
- Greene, B.L. and Wolf, S.L. (1989). Upper extremity joint movement: Comparison of two measurement devices. *Arch Phys Med Rehabil*, 70, 288-290.
- Grieve, D.W., Miller, D.I., Mitchelson, D. Paul, J.P., and Smith, A.J. (1975). *Techniques for the analysis of human movement*. Princeton, N.J.: Princeton Book Co. 177.
- Habes, D., Carlson, W. & Badger, D. (1985). Muscle Fatigue Associated with Repetitive Arm Lifts: effects of height, weight and reach. *Ergonomics*, 28 (2), 471-488.
- Hagg, G., Oster, J., Bystrom, S. (1996). Forearm muscular load and wrist angle among automobile assembly line workers in relation to symptoms. *Applied Ergonomics*, 28, 41-47.

- Hagberg, M. (1981). Work load and fatigue in repetitive arm elevations. *Ergonomics*, 24 (7), 543-555.
- Hennekens, C.H. and Buring, J.E. (1987). *Epidemiology in medicine*. Boston, Mass. Little, Brown and Co. 258-271.
- Herberts, P., Kadefors, R. and Broman, H. (1980). Arm positioning in manual tasks: An electromyographic study of localized muscle fatigue. *Ergonomics* 23 (7), 655-665.
- Herrin, G.D., Jariedi, M. and Anderson, C.K. (1986). Prediction of overexertion injuries using biomechanical and psychophysical models. *American Industrial Hygiene Association Journal*, 47, 322-330.
- Honsa, K., Vennettilli, M., Mott, N., Silvera, D., Neichwiej, E., Wagar, S., Howard, M., Zettel, J. and McGill, S. (1998). The efficacy of the NIOSH (1991) hand-to-container coupling factor. In, *Proceedings of the 30th Annual Conference of the Human Factors Association of Canada*.
- Industrial Engineer (2003). Cost of workplace injuries grows. *IE Engineering and Management solutions at work*, 35 (6), 9.
- Jager, M. and Luttman, A. (1989). Biomechanical analysis and assessment of lumbar stress during load lifting using a dynamic 19-segment human model. *Ergonomics*, 32, 93-112.
- Jager, M. and Luttman, A. (1991). Compressive strength of lumbar spine elements related to age, gender, and other influencing factors. In *A Guide to Manual Materials Handling*. Mital, A., Nicholson, A.S., and Ayoub, M.M. (1993). Washington, DC. Taylor & Francis, Inc.
- Jonsson, B. (1982). Measurement and evaluation of local muscular strain in the shoulder during constrained work. *Journal of Human Ergology*, 11, 73-88.
- Joseph, B., Reeve, G., Kilduff, H.A., Hall-Counts, J. and Long, M. (2000). Key elements of an ergonomics process: Developing surveillance tools to evaluate risk factors. *Proceedings of the IEA 2000/HFES 2000 Congress*.
- Kadefors, R., Peterson, I. & Herberts, P. (1976). Muscular reaction to welding work: An electromyographic investigation. *Ergonomics*, 19 (5), 543-558.
- Karhu, P., Kansi, P. and Kuorinka, I. (1977). Correcting working postures in industry: A practical method for analysis. *Applied Ergonomics*, 8 (4), 199-201.
- Karwowski, W. and Yates, J.W. (1986). Reliability of the psychophysical approach to manual lifting of liquids by females. *Ergonomics*, 29 (2), 237-248.
- Karwowski, W. and Brokaw, N. (1992). Implications of the proposed revisions in the draft of the revised NIOSH lifting guide (1991) for job redesign: a field study. *Proceedings of the Human Factors and Ergonomics Society 36th Annual Meeting*, 659-663.
- Keyserling, W., Stetson, D., Silverstein, B., and Brouwer, M. (1993). A checklist for evaluating ergonomic risk factors associated with upper extremity cumulative trauma disorders. *Ergonomics*, 36 (7), 807-831.

- Keyserling, W.M. and Chaffin, D.B. (1986). Occupational ergonomics- Methods to evaluate physical stress on the job. *Annual Review of Public Health*, 7, 77-104.
- Keyserling, W., Stetson, D., Silverstein, B., and Brouwer, M. (1993). A checklist for evaluating ergonomic risk factors associated with upper extremity cumulative trauma disorders. *Ergonomics*, 36 (7), 807-831.
- Kilbom, A. (1994)a. Repetitive work of the upper extremity: Part I – Guidelines for the practitioner. *International Journal of Industrial Ergonomics*, 14, 51-57.
- Kilbom, A. (1994)b. Repetitive work of the upper extremity: Part II - The scientific basis (knowledge base) for the guide. *International Journal of Industrial Ergonomics*, 14, 59-86.
- Kleinman, K, Lazarus, R. and Platt, R. (2004). A generalized linear mixed models approach for detecting incident clusters of disease in small areas, with an application to biological terrorism. *American Journal of Epidemiology*, 159 (3), 217-224.
- Konz, S. (1995). *Work design: Industrial ergonomics*. Scottsdale, AZ: Publishing Horizons, Inc.
- Krawczyk, S. (1993). Psychophysical determination of work design guidelines for repetitive upper extremity transfer tasks over an eight hour day. [Dissertation]. Ann Arbor, Mi: The University of Michigan.
- Krawczyk, S., Armstrong, T.J. and Snook, S.H. (1993). Psychophysical assessment of simulated assembly line work: Combinations of transferring and screw driving tasks. In proceedings of the Human Factors and Ergonomics Society, 37th annual meeting, Seattle, WA.
- Kroemer, K.H.E. (1989). Cumulative trauma disorders: Their recognition and ergonomic measures to avoid them. *Applied Ergonomics*, 20 (4), 274-280.
- Krom, M., Kester, A., Knipschild, P., Spaans, F. (1990). Risk Factors for Carpal Tunnel Syndrome. *American Journal of Epidemiology*, 132 (6), 1102-1110.
- Kromodihardjo, S. and Mital, A. (1986). Kinetic analysis of manual lifting activities: Part I – Development of a three-dimensional computer model. *International Journal of Industrial Ergonomics*, 1, 77-90. In *A Guide to Manual Materials Handling*, Mital, A., Nicholson, A.S. and Ayoub, M.M. (1993). Washington, DC. Taylor & Francis Inc.
- Kromodihardjo, S. and Mital, A. (1987). Biomechanical analysis of manual lifting tasks. *Journal of Biomechanical Engineering*, 109, 132-138. In *A Guide to Manual Materials Handling*, Mital, A., Nicholson, A.S. and Ayoub, M.M. (1993). Washington, DC. Taylor & Francis Inc.
- Kvarnstrom, S. (1983). Occurance of musculoskeletal disorders in the manufacturing industry with special attention to occupational shoulder disorders. *Scandinavian Journal of Rehabilitation Medicine*, 8, 111-114.
- Latko, W., Armstrong, T., Foulke, J., Herrin, G., Raybourn, R., Ulin, S. (1997). Development and evaluation of an observational method for assessing repetition in hand tasks. *American Industrial Hygiene Association Journal*, 58, 278-285.

- Lee, C-C., Nelson, E., Davis, K., and Marras, W. (1997). An ergonomic comparison of industrial spray paint guns. *International Journal of Industrial Ergonomics*, 19, 425-435.
- Leedy, P. and Ormrod, J. (2001). *Practical research*, seventh edition. Columbus, OH. Merrill Prentice Hall.
- Legg, S.J. and Myles, W.S. (1981). Maximum acceptable repetitive lifting workloads for an 8-hour workday using psychophysical and subjective rating methods. *Ergonomics*, 24 (12), 907-916.
- Legg, S.J. and Myles, W.S. (1985). Metabolic and cardiovascular cost, and perceived effort over an 8-hour day when lifting loads selected by the psychophysical method. *Ergonomics*, 28 (1), 337-343.
- Ljungberg, A.S., Gamberale, F. and Kilbom, A. (1982). Horizontal lifting- Physiological and psychological responses. *Ergonomics*, 25 (8), 741-757.
- Ljunggren, G. (1986). Observer ratings of perceived exertion in relation to self ratings and heart rate. *Applied Ergonomics*, 17 (2), 117-125.
- Loslever, P. and Ranaivosoa, A. (1993). Biomechanical and epidemiological investigation of carpal tunnel syndrome at workplaces with high risk factors. *Ergonomics*, 36 (5), 537-554.
- Marras, W. & Schoenmarklin, R. (1993). Wrist motions in industry. *Ergonomics*, 36 (4), 341-351.
- Marras, W., Marklin, R., and Greenspan, G. (1995). Quantification of wrist motions during scanning. *Human Factors*, 37 (2), 412-423.
- Marras, W.S., Lavender, S.A., Leurgans, S.E., Fetahallah, F.A. and Allread, W.G. (1995). Biomechanical risk factors for occupationally-related low back disorders. *Ergonomics*, 38 (2), 377-410.
- McAtamney, L., and Corlett, N. (1993). RULA: a survey method for the investigation of work-related upper limb disorders. *Applied Ergonomics*, 24, (2), 91-99.
- Merletti, R., LoConter, L.R. and Orizio, C. (1991). Indices of muscle fatigue. *Journal of Electromyography and Kinesiology*, 1 (1), 20-33.
- Merriam-Webster's (1993). *Merriam Webster's collegiate dictionary*, tenth edition. Springfield, MA. Merriam-Webster Inc.
- Michael, E.D., Hutton, K.E., and Horvath, S.M. (1961). Cardiorespiratory responses during prolonged exercise. *Journal of Applied Physiology*, 16, 997-999.
- Mital, A. (1983). Maximum frequencies acceptable to males for one handed horizontal lifting in the sagittal plane. *Human Factors*, 25 (5), 563-571.

- Mital, A. (1984a). Comprehensive maximal acceptable weight of lift database for regular 8-hour workshifts. *Ergonomics*, 27, 1127-1138. In, Mital, A. Nicholson, A. S., and Ayoub, M. M. (1993). *A guide to manual materials handling*. Washington, DC. Taylor and Francis, Inc.
- Mital, A. (1985). A comparison between psychophysical and physiological approaches across low and high frequency ranges. *Journal of Human Ergology*, 14, 59-64.
- Mital, A., Fard, H., Khaldei, H. and Channaveeraiah, C. (1987). Are manual lifting weight limits based on the physiological approach realistic and practical? In *Trends in Ergonomics/Human Factors IV*, edited by S.S. Asfour, pp 973-977. Amsterdam: North-Holland.
- Mital, A. (1992). Psychophysical capacity of industrial workers for lifting symmetrical and asymmetrical loads symmetrically and asymmetrically for 8-hour work shifts. *Ergonomics*, 35, 745-754.
- Mital, A. Nicholson, A. S., and Ayoub, M. M. (1993). *A guide to manual materials handling*. Washington, DC. Taylor and Francis, Inc.
- Moore, A., Wells, R. and Ranney, D. (1991). Quantifying exposure in occupational manual tasks with cumulative trauma disorder potential. *Ergonomics*, 34 (12), 1433-1453.
- Moore, S. and Garg, A. (1995). The Strain Index: A proposed method to analyse jobs for risk of distal upper extremity disorders. *American Industrial Hygiene Association*, 56, 443-458.
- Mugleton, J.M., Allen, R. and Chappell, P.H. (1999). Hand and arm injuries associated with repetitive manual work in industry: a review of disorders, risk factors and preventive measures. *Ergonomics*, 42 (5), 714-739.
- National Academy of Sciences (NAS) (1998). *Work related musculoskeletal disorders: A review of the evidence*. Washington, DC. National Academy Press.
- National Institute for Occupational Safety and Health (NIOSH) (1981). *Technical report: Work practices guide for manual lifting*. DHHS (NIOSH) publication No. 81-122.
- National Institute for Occupational Safety and Health (NIOSH) (1986). *Proposed national strategies for the prevention of leading work-related diseases and injuries: part 1*. Washington, DC: Association of Schools of Public Health.
- National Institute for Occupational Safety and Health (NIOSH) (1997). *Hazard evaluation and technical assistance report # TA 76-93 by Wisseman, C.L. and Badger, D.* Cincinnati, Ohio: US Department of Health, Education and Welfare, Center for Disease Control.
- National Institute for Occupational Safety and Health (NIOSH) (1997). *Musculoskeletal disorders and workplace factors*. DHHS (NIOSH) publication No. 97-141.
- Occupational Safety and Health Administration (OSHA) (1995). *Ergonomic protection standard*. Washington, DC.

- Occupational Safety and Health Administration (OSHA) (1999). Proposed rules, Department of Labor, Occupational Safety and Health Administration. Federal Register, 64 (225), 65768-66078.
- Oxenburgh, M. (1991). Increasing productivity and profit through health and safety. CCH International, North Ryde, N.S.W.
- Park, K. (1973). A computerized simulation model of postures during manual materials handling. PhD dissertation, University of Michigan, Ann Arbor, MI.
- Potvin, J.R. (1997). Effects of muscle kinematics on surface EMG amplitude and frequency during fatiguing dynamic contractions. *The American Physiological Society*, 0161-7567, 144-151.
- Potvin, J.R. & Bent, L.R. (1997). A validation of techniques using surface EMG signals from dynamic contractions to quantify muscle fatigue during repetitive tasks. *Journal of Electromyography and Kinesiology*, 7 (2), 131-139.
- Potvin, J.R. & Bent, L.R. (1997). NIOSH equation horizontal distances associated with the Liberty Mutual (Snook) lifting table box widths. *Ergonomics*, 40 (6), 650-655.
- Potvin, J.R., Dawson, D., MacPherson, M. and Joseph, B. (2002a). Evaluating the ACGIH TLV guideline for low force/high frequency work. *The Proceeding of the XVI Annual International Occupational Ergonomics and Safety Conference*.
- Potvin, J.R., Dawson, D., Jones, J., MacPherson, M. and Joseph, B. (2002b). Comparing risk-scores from the ACGIH TLV guideline when obtained from live observation and video records. *The Proceeding of the XVI Annual International Occupational Ergonomics and Safety Conference*.
- Putz-Anderson, V. (1988)a. Prevention strategies adopted by select countries for work-related musculoskeletal disorders from repetitive trauma. In *Trends in Ergonomics/Human Factors V*, edited by F.Aghazadeh. North-Holland: Elsevier Science Publishers, 601-611.
- Putz-Anderson, V. (1988)b. *Cumulative Trauma Disorders: Manual for musculoskeletal diseases of the upper limbs*. Bristol, PA: Taylor & Francis.
- Radwin, R.G., Masters, G.P. and Lupton, F.W. (1991). A linear force-summing hand dynamometer independent of point of application. *Applied Ergonomics*, 22 (5), 339-345.
- Reed H., Peacock, B. and Mohr, E. (1999). The frequency factor in manual lifting. *Applied Ergonomics Case Studies*, Volume 2. 66-79.
- Rempel, D., Harrison, R., & Barnhart, S. (1992). Work-related cumulative trauma disorders of the upper extremity. *Journal of the American Medical Association*, 267, 838-842.
- Rodgers, S.H., Yates, J.W. and Garg, A. (1991). The physiological basis for manual lifting guidelines. National Technical Information Service, Report No. 91, 227-330.
- Rodgers, S.H. (1992). A functional job analysis technique. *Occupational Medicine: State of the art reviews*. April-June, 3 (2).

- Rohmert, W. (1973). Problems in determining rest allowances. Part 2 - Determining rest allowances in different human tasks. *Applied Ergonomics*, 4 (2), 158-162.
- Rose, L., Ericson, M., Glimskar, B., Nordgren, B. & Ortengren, R. (1992). Ergo-Index. A model to determine pause needs after fatigue and pain reactions during work. *Advances in Industrial Ergonomics and Safety IV*, 303-310.
- Rosecrance, J.C. and Cook, T.M. (1998). Upper extremity musculoskeletal disorders: Occupational association and a model for prevention. *Central European Journal of Occupational and Environmental Medicine*, 4 (1), 214-231.
- Sanders, M.S. and McCormick, E.J. (1993). *Human factors in engineering and design*. New York, NY: McGraw Hill.
- Schoenmarklin, R., Marras, W. (1993). Dynamic capabilities of the wrist joint in industrial workers. *International Journal of Industrial Ergonomics*, 11, 207-224.
- Schoenmarklin, R., Marras, W., Leugans, S. (1994). Industrial wrist motions and incidence of hand/wrist cumulative trauma disorders. *Ergonomics*, 37 (9), 1449-1459.
- Selan, J. (1994). *The Advanced Ergonomic Manual*. Dallas, TX: Advanced Ergonomics Inc.
- Silverstein, B. (1985). *The prevalence of upper extremity cumulative trauma disorders in industry [Dissertation]*. Ann Arbor, Mi: The University of Michigan.
- Silverstein, B.A., Fine, L.J. and Armstrong, T.J. (1987). Occupational factors and carpal tunnel syndrome. *American Journal of Industrial Medicine*, 11, 343-358.
- Skrondal, A. and Rabe-Hesketh, S. (2003). Some applications of generalized linear latent and mixed models in epidemiology: Repeated measures, measurement error and multilevel modeling. *Norsk Epidemiologi*, 13 (2), 265-278.
- Snook, S.H. and Irvine, C.H. (1968). Maximum frequency of lift acceptable to male industrial workers. *American Industrial Hygiene Association Journal*, 29, 531-536.
- Snook, S.H. and Irvine, C.H. (1969). Psychophysical studies of physiological fatigue criteria. *Human Factors*, 11 (3), 291-300.
- Snook, S., Irvine, C., and Bass, S. (1970). Maximum weights and work loads acceptable to male industrial workers: A study of lifting, lowering, pushing, pulling, carrying, and walking tasks. *American Industrial Hygiene Association Journal*, 31, 579-586.
- Snook, S. H. (1978). The design of manual handling tasks. *Ergonomics*, 21 (12), 963-985.
- Snook, S.H. (1985). Psychophysical acceptability as a constraint in manual working capacity. *Ergonomics*, 28 (1), 331-335.
- Snook S.H. and Ciriello, V.M., (1991) The design of manual handling tasks: Revised tables of maximum acceptable weight and forces. *Ergonomics*, 34 (9), 1197-1213.

- Snook, S., Vaillancourt, D., Cirello, V., Webster, B. (1995). Psychophysical studies of repetitive wrist flexion and extension. *Ergonomics*, 38 (7), 1488-1507.
- Snook, S., Vaillancourt, D., Cirello, V., Webster, B. (1997). Maximum acceptable forces for repetitive ulnar deviation of the wrist. *American Industrial Hygiene Association Journal*, 58, 509-517.
- Sommerich, C., McGlothlin, J., and Marras, W. (1993). Occupational risk factors associated with soft tissue disorders of the shoulder: a review of recent investigations in literature
- Sommerich, C., Marras, W., and Parnianpour, M. (1996). A method for developing biomechanical profiles of hand-intensive tasks. *Clinical Biomechanics*, 13, 261-271.
- Spatz, C. and Johnston, J. (1989). *Basic Statistics, tales of distributions*, 4th edn. Cole Publishing Co. Pacific Grove, C.A. 395.
- Stock, S. (1991). Workplace ergonomic factors and development of musculoskeletal disorders of the neck and upper limbs: a meta-analysis. *American Journal of Industrial Hygiene*, 19, 87-107.
- Suurkula, J. and Hagg, G. (1987). Relations between shoulder/neck disorders and EMG zero crossing shifts in female assembly workers using the test contraction method. *Ergonomics*, 30 (11), 1553-1564.
- Tolmie, S.W. (2002). An evaluation of the validity and reliability of an ergonomic risk factor checklist. Thesis. University of Windsor. Windsor, Ontario, Canada.
- Topp, K. and Byl, N. (1999). Movement dysfunction following repetitive hand opening and closing: Anatomical analysis in owl monkeys. *Movement Disorders*, 14 (2), 295-306.
- Tracy, M.F. (1990). Biomechanical methods in posture analysis. In *Evaluation of Human Work*, edited by John R. Wilson and E. Nigel Corlett. New York, NY: Taylor & Francis, Inc. 571-604.
- Troup, J.D., Martin, J.W. and Lloyd, C.E.F. (1981). Back pain in industry: A prospective survey. *Spine*, 6, 61-69.
- UAW-Ford Motor Company (1999). Contractual working agreement. Appendix S. Bulletin number 1.0. Standard methods and guidelines for UAW-Ford Local Ergonomic Committees.
- University of Michigan (2000). University of Michigan 3DSSPP 4.21.
- U.S. Department of Health and Human Services (DHHS). (1992). Selected topics in surface electromyography for use in the occupational setting: Experts perspectives. DHHS (NIOSH) Publication No. 91-100.
- U.S. General Accounting Office (GAO) Health Education and Human Services (HEHS). (1997). Worker protection – Private sector ergonomics programs yield positive results. GAO/HEHS Publication No. 97-163.

- Vi, P. (1998). Evaluation of the frequency distribution and validity of the NIOSH recommended weight limit. Proceedings of the 30th Annual Conference of the Human Factors Association of Canada.
- Vollestad, N.K. (1997). Measurement of human muscle fatigue. *Journal of Neuroscience Methods*, 74, 219-227.
- Waly, S.M., Kahlil, T.M. and Asfour, S.S. (1986). Physiological basis of muscular fatigue: An electromyographic study. *Trends in Ergonomics/Human Factors III*, 751-758.
- Waters, T.R., Putz-Anderson, V., Garg, A. and Fine, L.J. (1993). Revised NIOSH equation for the design and evaluation of manual lifting tasks. *Ergonomics*, 36 (7), 749-776.
- Wardle, M.G. and Gloss, D.S. (1978). A psychophysical approach to estimating endurance in performing physically demanding work. *Human Factors*, 29 (6), 745-747.
- Weir, J.B. (1949). New methods for calculating metabolic rate with special reference to protein metabolism. In Garg, A., Chaffin, D.B. and Herrin, G. (1978). Prediction of metabolic rates for manual materials handling jobs. *American Industrial Hygiene Association Journal*, 39 (8), 661-674.
- Wells, R., Moore, A., Potvin, J. and Norman, R. (1994). Assessment of risk factors for development of work-related musculoskeletal disorders (RSI). *Applied Ergonomics*, 25 (3), 157-164.
- Winkel, J. & Westgaard, R. (1992)a. Occupational and individual risk factors for shoulder-neck complaints: Part I – Guidelines for the practitioner. *International Journal of Industrial Ergonomics*, 10, 79-84.
- Winkel, J. & Westgaard, R. (1992)b. Occupational and individual factors for shoulder-neck complaints: Part II - The scientific basis (literature review) for this guide. *International Journal of Industrial Ergonomics*,
- Worker's Compensation Board (WCB) (1994). Issued by : The Secretariat for Regulation Review Board of Governors, Draft Ergonomics Regulations. Vancouver, BC: WCB.
- World Health Organization (1989). Identification and control of work-related diseases. WHO Technical Report Series
- Yamada, H., Kiryu, T. and Okada, M. (2001). Development of muscle fatigue assessed by using superposition of eveoked and volitional myoelectrical potentials. *Perceptual and Motor Skills*, 93, 3-10.
- Yoshitake, H. (1971). Relations between the symptoms and the feeling of fatigue. *Ergonomics*, 14 (1), 175-186.
- Zetterberg, C. and Ofverholm, T. (1999). Carpal tunnel syndrome and other wrist/hand symptoms and signs in male and female car assembly workers. *International Journal of Industrial Ergonomics*, 23, 193-204.

APPENDIX A



LETTER OF INFORMATION

Evaluation of the reliability of an ergonomic decision system

You are asked to participate in a research study conducted by: Dr. Jim Potvin and Derek Dawson

If you have any questions or concerns about the research, please feel to contact either:

1. Dr. Jim Potvin, Associate Professor, Faculty of Human Kinetics, University of Windsor (519-253-3000 x2461; Room 117 HK Building; jpotvin@uwindsor.ca) or home: 967-0233.

2. Derek Dawson, Ergonomic Engineer, Ford Motor Company (313-248-7209; Room E1280 Ford Motor Company, VOGO, Dearborn, MI, 48121;

PURPOSE OF STUDY

The purpose of this research is to establish the reliability and validity of a unique ergonomic process, deemed the Ergonomic Decision System. Though based on universally applicable research, the EDS was designed to be used within the automotive manufacturing sector.

Validity will be established via an in-depth literature review, from which the content of decision system was developed. Between and within-rater reliability of the decision system will be established from controlled lab testing with a number of trained and untrained engineers working in isolation, under time restrictions and using the process in an attempt to analyze several jobs

Reliability studies produce two results. The first is that the trained individuals, using the EDS will repeatedly choose the same and most applicable ergonomic tool for analysis. Second, that the results of the use of the tool indicate true positive and true negative conditions. That is to say, it is desirable to avoid conditions where an element of an operation is labeled as ergonomically unsuitable when in reality it is sound (false positive). Or conversely and perhaps more importantly, the labeling of an element of an operation as ergonomically suitable when it is in fact not (false negative).

PROCEDURES

Each of twelve subjects (6 expert and 6 novice) will each receive like verbal instructions on the test procedure. Subjects will be provided a work-station containing a computer, ergonomic decision system and HyperCam[®] software. Subjects will then be shown a video segment from an industrial work setting containing several full cycles of the assembly operations being evaluated.

The subject will be able to request repeated viewing of the work tasks. Further, upon request the subjects will be provided any pertinent, additional information regarding to the operation.

In order to assess between-rater reliability, subjects will be presented with six full assembly operations. three operations were chosen from each of the two automotive assembly facilities. Although each of the operations contain many different risk-factors, four of the total six were selected in order assess a predominant action or posture. The remaining two represent variations of one of the original four actions and postures. The rationale for the action or posture duplication with variations are to provide the subject with a variety of conditions which may require analysis within an assembly facility and to assess the decision process under these conditions.

After a minimum of two weeks post-test each of the twelve subjects will repeat the analysis of one randomly chosen operation. Results between the original analysis and second will provide information for within-subject reliability comparisons.

All ergonomic decision system software use will be simultaneously recorded using HyperCam[®] software. These recordings will provide information on time required to complete tasks and decision paths chosen. This will then be compared to the most accurate and succinct analysis method as established by select and non-participatory expert consensus agreement.

POTENTIAL RISKS AND DISCOMFORTS

Results of the subjects analysis of the six operations will be kept confidential, however the chance exists that participants may discuss the operations. This may lead to some level of disagreement and perhaps emotional issues at some level. Please contact Dr. Potvin (519-253-3000 ext 2461) if you have any questions or concerns.

POTENTIAL BENEFITS TO SUBJECTS AND/OR TO SOCIETY

The results of the study will benefit industrial workers within the automotive community. Ford Motor Company will use the results to determine applicability of the decision system for use by a variety of audiences both proactively and reactively within its assembly facilities. The goal is to ensure that the use of the ergonomic decision system reduce the potential for injury or illness in automotive manufacturing.

PAYMENT FOR PARTICIPATION

Participants will be recruited on a volunteer basis.

CONFIDENTIALITY

Any information that is obtained in connection with this study and that can be identified with you will remain confidential and will be disclosed only with your permission. Only the researchers mentioned above will know your identity and personal information. This information will be stored in a secure computer in the ergonomics simulation laboratory (VOGO) and will not be discussed or displayed in any form that would provide an indication of your identity.

Note that subjects should not converse with other participants about the software, analysis and/or results as this may offend some and may further bias future collections.

PARTICIPATION AND WITHDRAWAL

You can choose whether to be in this study or not. If you volunteer to be in this study, you may withdraw at any time without consequences of any kind. You may exercise the option of removing your data from the study. You may also refuse to answer any questions you don't want to answer and still remain in the study. The investigator may withdraw you from this research if circumstances arise which warrant doing so.

RIGHTS OF RESEARCH SUBJECTS

You may withdraw your consent at any time and discontinue participation without penalty. This study has been reviewed and received ethics clearance through the University of Windsor Research Ethics Board. If you have questions regarding your rights as a research subject, contact:

Research Ethics Co-ordinator

Telephone: 519-253-3000, # 3916
University of Windsor
E-mail:

Windsor, Ontario
N9B 3P4



CONSENT TO PARTICIPATE IN RESEARCH

SIGNATURE OF RESEARCH SUBJECT/LEGAL REPRESENTATIVE

I understand the information provided for the study "Evaluation of the reliability of an ergonomic decision system" as described herein. My questions have been answered to my satisfaction, and I agree to participate in this study. I have been given a copy of the 'Letter of information' and 'Consent to participate in research' forms.

Subjects will receive feedback on the results of the experiment by way of a feedback form. This form will be filled out by the investigators, including the major findings and implementations of the study.

Name of Subject

Signature of Subject

Date

SIGNATURE OF INVESTIGATOR

These are the terms under which I will conduct my research.

Signature of Investigator
Derek I. Dawson

Date

Advisor, Dr. J. Potvin

APPENDIX B

Novice Survey

Q1 – What does the word Ergonomics mean?

A1 – The study of work

Q2 – What are two approaches to addressing workplace conditions?

A2 – Proactive & Reactive

Q3 – What is meant by a workplace risk factor (with regard to Ergonomics)?

A3 – A work element &/or action that increases the workers risk of injury/illness

Q4 – What are the three main risk factors from an Ergonomic perspective?

A4 – Force, posture, repetition

Q5 – What does the term CTD stand for?

A5 – Cumulative trauma disorder

Q6 – When designing for reach, what population percentile would you minimally design for?

A6 – 5th percentile female

Q7 – What population percentile is used to set force design standards?

A7 – 25th percentile female (90th percentile population)

Q8 – What does OSHA stand for?

A8 – Occupational Safety & Health Administration

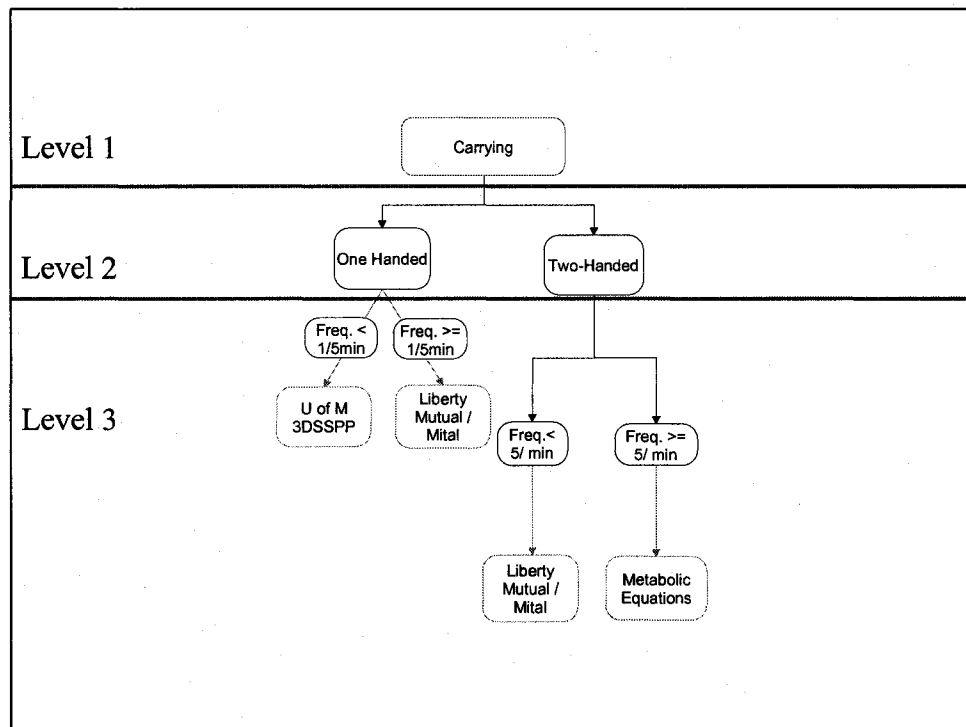
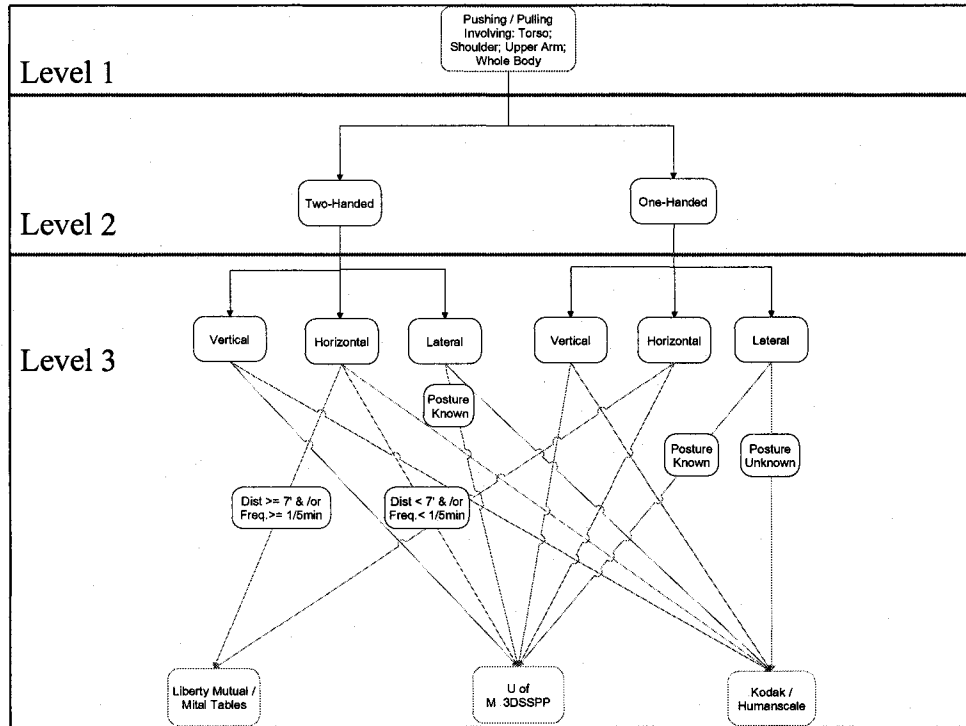
Q9 – Work rotation is an example of what type of control?

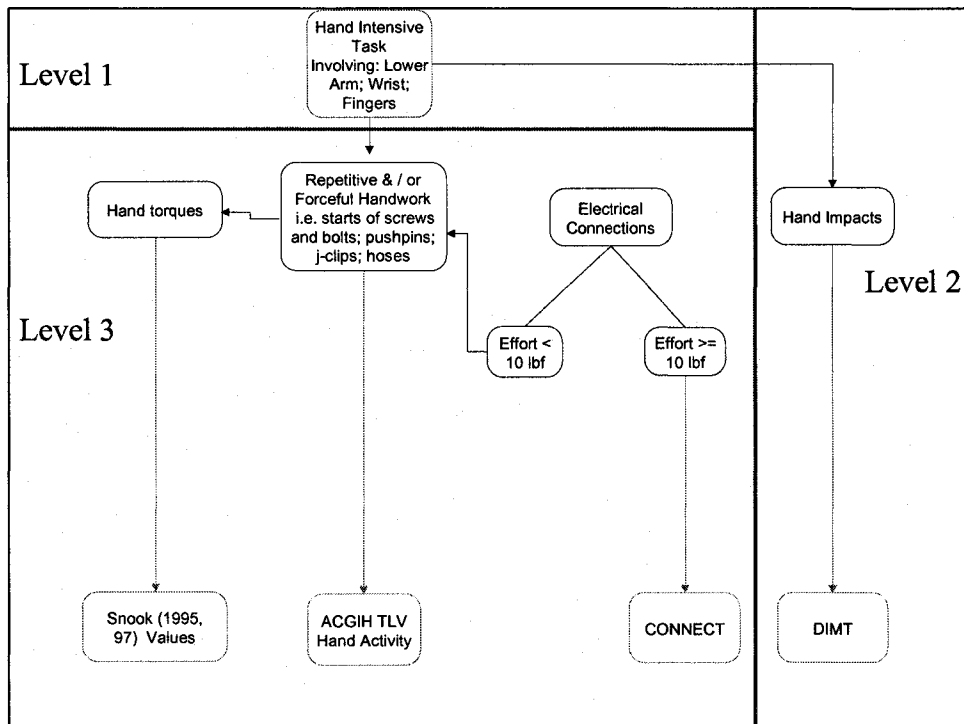
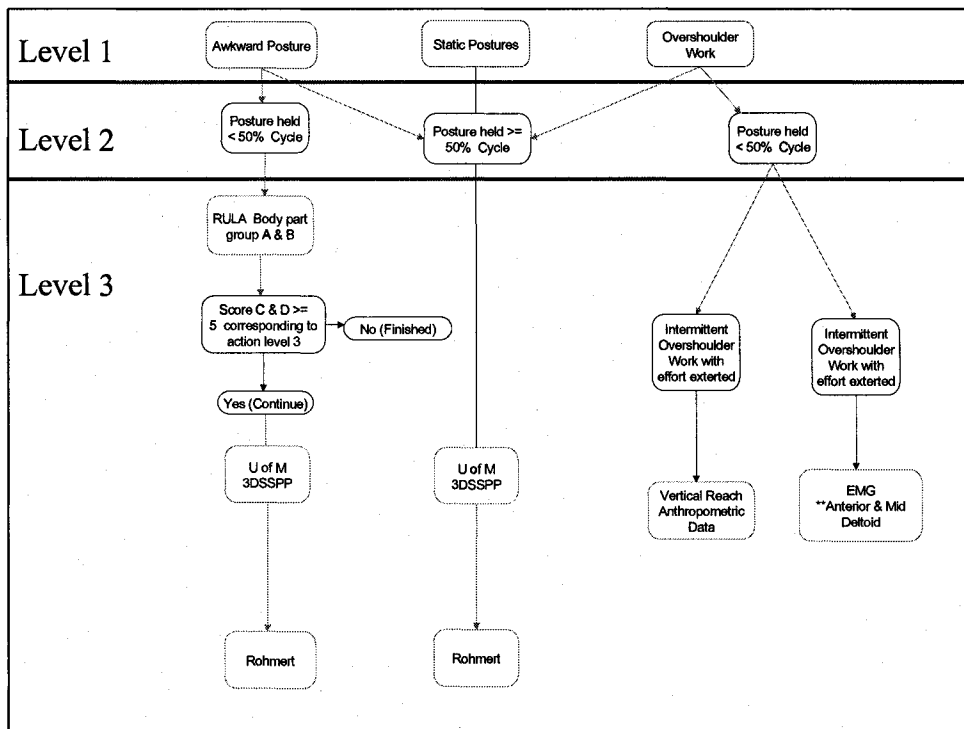
A9 - Administrative

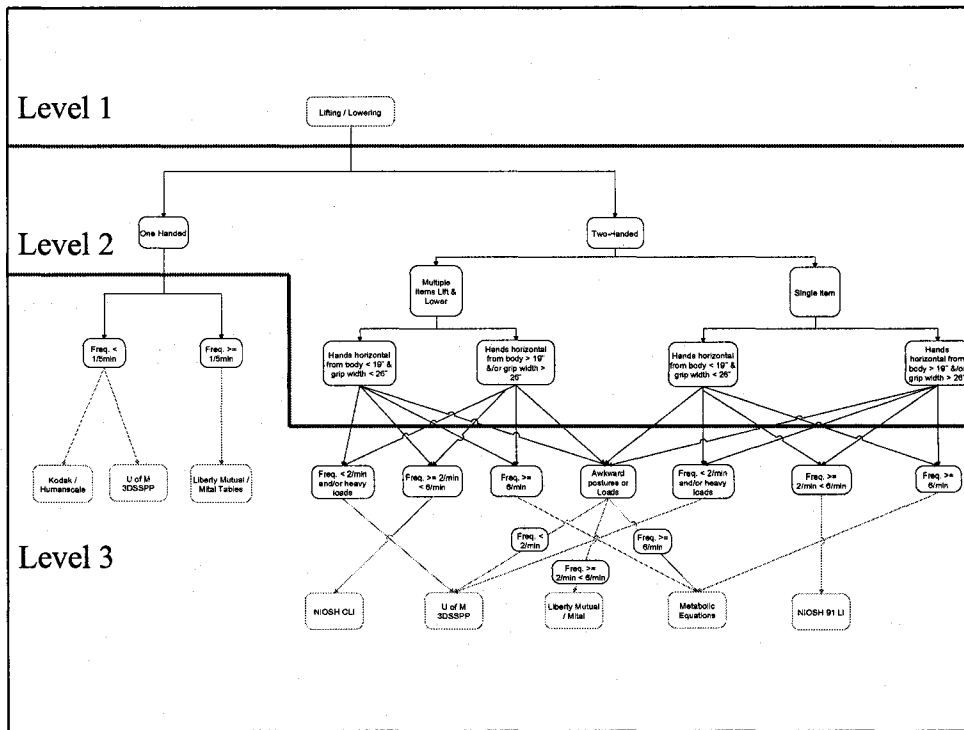
Q10 – True or False – As frequency of movement increases, force requirements should decrease?

A10 - True

APPENDIX C EDS FLOWCHART







VITA AUCTORIS

NAME: Derek Ian Dawson

PLACE OF BIRTH: Lachine, Quebec, Canada

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1985 – 1990 O.S.S.G.D.

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