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Micro and Nano Mechanical Testing of Materials and Devices

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1 Deformation behavior of nanoporous metals

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1.1 Introduction

Nanoporous open-cell foams are a rapidly growing class of high-porosity materials (porosity \geq 70%). The research in this field is driven by the desire to create functional materials with unique physical, chemical and mechanical properties where the material properties emerge from both morphology and the material itself. An example is the development of nanoporous metallic materials for photonic and plasmonic applications which has recently attracted much interest. The general strategy is to take advantage of various size effects to introduce novel properties. These size effects arise from confinement of the material by pores and ligaments, and can range from electromagnetic resonances [1] to length scale effects in plasticity.[2, 3]

In this chapter we will focus on the mechanical properties of low density nanoporous metals and how these properties are affected by length scale effects and bonding characteristics. A thorough understanding of the mechanical behavior will open the door to further improve and fine-tune the mechanical properties of these sometimes very delicate materials, and thus will be crucial for integrating nanoporous metals into products. Cellular solids with pore sizes above 1 micron have been the subject of intense research for many years, and various scaling relations describing the mechanical properties have been developed.[4] In general, it has been found that the most important parameter in controlling their mechanical properties is the relative density, that is, the density of the foam divided by that of solid from which the foam is made. Other factors include the mechanical properties of the solid material and the foam morphology such as ligament shape and connectivity. The characteristic internal length scale of the structure as determined by pores and ligaments, on the other hand, usually has only little effect on the mechanical properties. This changes at the submicron length scale where the surface-to-volume ratio becomes large and the effect of free surfaces can no longer be neglected. As the material becomes more and more constraint by the presence of free surfaces, length scale effects on plasticity become more and more important and bulk properties can no longer be used to describe the material properties. Even the elastic properties may be affected as the reduced coordination of surface atoms and the concomitant redistribution of electrons may soften or stiffen the material. If, and to what extend, such length scale effects control the mechanical behavior of nanoporous materials depends strongly on the material and the characteristic length scale associated with its plastic deformation. For example, ductile materials such as metals which deform via dislocation-mediated processes can be expected to exhibit pronounced length scale effects in the sub-micron regime where free surfaces start to constrain efficient dislocation multiplication. In this chapter we will limit our discussion to our own area of expertise which is the mechanical behavior of nanoporous open-cell gold foams as a typical example of nanoporous metal foams. Throughout this chapter we will review our current understanding of the mechanical properties of nanoporous open-cell foams including both experimental and theoretical studies.

1.2 Processing Techniques

Nanoporous metal foams have been made in various shapes such as nanowires, [5, 6] thin-films, [7, 8] and macroscopic 3D samples. [8, 9] Their morphology ranges from disordered three-dimensional network structures (sponge-like morphology) to well-defined periodic thin-film structures with excellent long-range order which are mostly used for photonic applications. This section provides a short review of the synthesis of nonperiodic nanoporous metal foams which can be prepared in the form of very uniform millimeter-sized 3D objects. A typical example of the sponge-like open-cell foam morphology of np-Au is shown in Figure 1a.

Synthesis techniques include top-down (dealloying) and bottom-up strategies (filter casting and templating) as well as combinations thereof. Many of these techniques have been developed or further refined at Lawrence Livermore National Laboratory with the ultimate goal to design a new class of three-dimensional nanoporous metals for high energy density laser experiments. This application requires the fabrication of millimetersized, defect-free monolithic samples of nanoporous materials with welldefined pore-size distributions (including hierarchical porosities) and adjustable densities down to a few atomic percent. Yet the material has to be mechanical robust enough to be machined. An example of such a Laser target is shown in Figure 1b.



Fig. 1. (*a*) Focused ion beam nanotomography (FIB-nt) image showing the 3Dstructure of nanoporous Au. This state-of-the-art FIB-nt image was collected by L. Holzer, Ph. Gasser and B. Münch from EMPA, Switzerland. The resolution of 2*3*6 nm presents the current record of the FIB-nt method, and allows one to determine microstructural parameters responsible for mechanical size effects of nanoporous materials. (*b*) Machined ultra-low density Au foam target for highenergy-density Laser experiments. The picture was provided by courtesy of Craig Akaba, LLNL

1.2.1. Dealloying

Dealloying is by far the most often applied method to generate macroscopic 3D as well as 2D (thin-film) and 1D (nanowire) samples of lowdensity nanoporous metal foams for nanomechanical testing. In metallurgy, dealloying is defined as selective corrosion (removal) of the less noble constituent from an alloy, usually via dissolving this component in a corrosive environment.[10, 11] In case of binary solid-solution alloys with a narrow compositional range around A_{0.7}B_{0.3} (where B is the less noble alloy constituent) this process can lead to spontaneous pattern formation, that is, development of a three-dimensional bicontinuous nanoporous structure while maintaining the original shape of the alloy sample. The material can be very uniform, even on a macroscopic length scale, and typically exhibits a specific surface area in the order of a few $m^2/g.[12]$ The best-studied example is the formation of nanoporous gold (np-Au) via selective removal of Ag from a AuAg alloy, [7, 8, 11] but other alloys such as AuAl₂,[13] MnCu (np-Cu),[14] and CuPt (np-Pt) [15] have also been successfully dealloyed. The process can be easily extended to twodimensional thin-film samples by using commercially available white-gold leaves with a thickness of a few hundred nanometers[7] or thin sputterdeposited alloy films.[16, 17] Even one-dimensional structures such as nanoporous Au nanowires can be fabricated by using combination of electrochemical templating and dealloying.[5] The characteristic sponge-like open-cell foam morphology of np-Au is illustrated by the focused ion beam nanotomography image shown in Figure 1a.

Nanoporous Au is ideally suited to study length scale effects in nanoporous metal foams due to its unique annealing behavior: The length scale of both pores and ligaments can easily be adjusted by a simple thermal treatment in ambient over a wide range from 3 nm to the micron length scale.[18-20] Most notably, the material rearrangement during annealing does not affect the relative density or relative geometry of the material (ligament connectivity or ligament, pore, and sample shape).[18, 21] An example of such an annealing experiment is shown in Figure 2.



Fig. 2. Cross-sectional SEM micrographs of as-prepared (ap) and annealed np Au: 300 °C, 500 °C, 700 °C. Note the self-similarity of the structure while increasing the feature size by more than a factor of 30. The relative density of the materials remains constant at approximately 30%

The dealloying technique can also be used to introduce even more complicated morphologies such as hierarchical porosities. For example, bimodal pore size distributions can be realized by using a 3-step dealloy-ing/annealing/dealloying strategy where a micon-scale ligament structure is first generated by dealloying followed by annealing, and nano-scale porosity is finally reintroduced into the ligaments by a second dealloying step. This approach requires either the use of a ternary alloys as starting material, or relies on metal deposition after the first dealloying/annealing step.[22] For example, we have used ternary Cu-Ag-Au alloys to prepare low-density (~10 at.% relative density) nanoporous Au samples with a bimodal pore size distribution. However, preparation of the appropriate homogeneous single phase ternary alloy is challenging and limits the applicability of this approach.

1.2.2. Bottom-up approaches

Although the bottom-up approach to nanostructured metal foams is very versatile regarding the range of accessible densities and morphologies, very little is known about the mechanical properties of the resulting materials. The technique usually involves the use of sacrificial organic materials such as polystyrene (PS) micro beads as templates to generate a nanostructured porous solid.[23, 24] The dimensions of the template directly determine the length scale of the porosity in the final structure. The technique also provides a powerful approach to create materials with complex hierarchical porosities, specifically in combination with dealloying.

In the case of Au foams, the synthesis starts with the preparation large quantities of Au or Ag-Au coated core-shell particles. These man-made building blocks are then assembled (casted) into a monolithic porous structure using a procedure analogous to the slip-casting process of ceramic [25] and metal [24] particles. Finally, the pure Au foam sample is obtained by removing the PS template by a simple heat treatment (Figure 3). If Ag-Au coated core-shell particles were used as a starting material one easily can introduce hierarchical porosities by adding a dealloying step. The technique out-lined above has been successfully used to fabricate millimeter-sized, defect-free monolithic samples of nanoporous Au with well-defined pore-size distributions and densities down to a few atomic percent (see for example the Laser target shown in Figure 1b).



Fig. 3. Ultra-low density metal foam (1g/cc) prepared from hollow 1 micron diameter Ag_{0.7}Au_{0.3} shells. The SEM micrograph was provided by courtesy of G.W. Nyce, LLNL

1.3. Deformation Behavior

1.3.1 Macroporous foams

Before going into further details on the deformation behavior of nanoporous foams, it is beneficial to cover the basics of foam mechanics. To keep this discussion short, we will only address the deformation behavior of open-cell foams. A complete discussion can be found in "Cellular Solids" by Gibson and Ashby.[4]

Our knowledge on foam mechanics comes almost exclusively from the study of macroporous foams with cell sizes exceeding one micron. As stated in the introduction, the behavior of such materials is governed by the properties of the base material and the porosity, or more specifically, the relative density (ρ^*/ρ_s) which is defined as the density of the foam (ρ^*) divided by the density of the material it is made of (ρ_s). A variety of scaling relations has been developed to predict and describe the properties of cellular solids using these two parameters. For example, by compiling experimental data collected from a wide variety of open-cell foams it can be shown that the yield strength (σ) and the Young's modulus (*E*) of open-cell foams can be described by the following scaling relations:

$$\sigma^* = C_2 \sigma_s \left(\frac{\rho^*}{\rho_s}\right)^{3/2} \tag{1}$$

$$E^* = C_1 E_s \left(\frac{\rho^*}{\rho_s}\right)^2 \tag{2}$$

where * refers to foam properties and *s* to the bulk properties, and $C_1=1$ and $C_2=0.3$ are fitting constants. It is important to notice that these scaling relations contain no explicit length scale dependence and assume that the material properties of the ligaments such as the yield strength and the Young's modulus are size-independent and equal to the bulk value. As will be discussed below, this assumption is no longer valid for metallic foams with submicron features.

Experimentally, the mechanical behavior of foams is typically studied in compression; however, tensile testing has been used as well.[26, 27] In the case of a uniaxial compression test the typical stress –strain deformation curve for an elastic-plastic foam will be composed of a linear elastic regime followed by a collapse plateau followed by a densification regime (Fig. 4).



Fig. 4. Representative compressive stress-strain behavior of a metal foam showing regimes of elastic and plastic deformation until densifications dominates

Indentation is another frequently used technique to assess hardness and yield strength data of cellular solids.[28-32] In the case of low-density foams ($\rho^*/\rho_s \leq 0.3$), it is generally assumed that the indentation hardness (*H*) is approximately equal to the yield strength, $H \sim \sigma_y$, rather than following the $H \sim 3\sigma_y$ relationship typically observed for fully dense materials.[4] The reason for this is that the material under the indenter is not constraint by the by the surrounding material as it densifies with very little lateral spread (which translates into an effective Poisson's ratio ~ 0). The $H \sim \sigma_y$ relationship has been validified by a number of studies, and is used throughout this review to assess the yield strength of low-density metal foams from nanoindentation hardness data. However, it has to be pointed out that this relationship is only valid for foams with at least 60% porosity and when issues such as indentation size effects and densification are properly accounted for. A detailed discussion on this topic can be found in a recent publication.[21]

1.3.2 Nanoporous Foams

In the case of nanoporous materials, the majority of studies have relied on nanoindentation as a tool to measure mechanical properties such as yield strength and Young's modulus.[33-35] The technique has the advantage of being experimentally simple and, compared to other techniques, of having relatively low requirements regarding sample size or defect concentration. Furthermore, nanoindentation can be easily applied to thin-films and irregularly shaped samples as long as the surface roughness is low. Other, experimentally more complex methods are pillar micro-compression tests [36, 37] and film or beam bending tests.[16, 35, 38, 39] Examples of nanoindentation, the yield strength is typically obtained by assuming that $\sigma_y \sim H$ as discussed above. Given that more studies have addressed the yield strength, we will start with a discussion of the yield strength data, followed by a short review on the elastic properties of nanoprous Au.

Strength and modulus

Nanoporous Au has been the preferred material in the majority of studies in this field.[21, 33-36, 40] As outlined above, the material is ideally suited to study length scale effects on plasticity in nanoporous metal foams as the pore size is experimentally simple to control, for example by annealing. Another material systems studied is nanoporous Cu.[14] The two most often reported properties are yield strength and elastic modulus, and the



Fig. 5. Typical examples of nanomechanical tests performed on nanoporous Au: (*a*) Series of nanoindentation load-displacement curves using a Berkovich tip (left) and a SEM micrograph showing a typical residual impression of such a test (right). This specific test was performed on nanoporous Au with a relative density of 0.25 and an average ligament width of 30 nm, and reveals a yield strength of 53 MPa. (*b*) Load-displacement curve of a deflective tensile test performed on microfabricated dog-bone samples (left). Curve fitting to non-linear beam theory reveals an elastic modulus of ~ 9GPa (relative density ~0.35, ligament width 20-40 nm). SEM micrograph of a dog-bone sample for deflective tensile tests (right). The tensile test data were provided by courtesy of J.W. Kysar, Columbia University (New York)

reported values for these properties range from 15 MPa to 240 MPa and 7 GPa to 40 GPa, respectively (Figure 6). Surprisingly, and despite its high porosity, nanoporous Au (240 MPa) can be stronger than bulk Au (200 MPa for severely worked single Au crystals). It is instructive to compare these values with the predictions made by the Gibson and Ashby scaling relations. One can calculate the yield strength and the Young's modulus of nanoporous Au as a function of relative density using Eqs. 1 and 2, and the bulk properties of Au as input. The yield strength of bulk Au is very dependent on the sample history, and values as low as 2 MPa for well-

annealed and as high as ~ 200 MPa for severely worked single crystals have been reported (see for example Ref. [41] and references wherein). To be conservative, we will use the high-end value of ~200 MPa, and the average value of the elastic modulus, ~ 80 GPa.[42] Assuming that the relative densities range from 25 to 42%, Eqs. 1 and 2 then predict yield strength values from 7.5 to 16 MPa and elastic modulus values from 5 to 14 GPa (see solid lines in Figure 6). Clearly, the experimental data do not follow the prediction made by the scaling relations: Specifically the yield strength data are higher than predicted, sometimes by more than an order of magnitude. The Young's modulus seems to be better described by the scaling equations, but the data are still very scattered. Furthermore, one can observe length scale effects not predicted by the Gibson and Ashby scaling relations. For example, the yield strength of nanoporous Au with relative density of 30% increases from ~10 MPa to ~ 100 MPa as the ligament sizes decreases from 900 nm to 40 nm.[21] In conclusion, only for the largest ligaments a reasonable agreement between experiment and theory is observed.



Fig. 6. Calculated (lines) and experimental (symbols) yield strength (*a*) and Young's modulus (*b*) data of nanoporous Au plotted as a function of the relative density of the material. Both yield strength and Young' modulus have been normalized using $\sigma_{solid} = 200$ MPa and $E_{solid} = 80$ GPa as the yield strength and Young's modulus of fully dense Au

To compile data obtained from samples with different relative densities and check for length scale effects, it is instructive to use equation 1 and 2 to calculate the mechanical properties of the ligament material, and plot the result as a function of the ligaments size. The result of such a data compilation is shown in Figure 7. Figure 7a reveals that the calculated strength of the ligament materials increases with decreasing feature size, independent of the testing method. This is in contrast to previous studies on macrocellular foams which found that for a given porosity the cell size had a minimal effect in the mechanical behavior.[43, 44] Clearly, this is not true for the nanoporous foams. In contrast, as revealed by Figure 7a, the majority of studies on nanoporous Au observe that the yield strength of the ligaments in nanoporous Au approaches the theoretical shear stress $G/2\pi$ of Au ~4.3 GPa) as the ligament size decreases to the 10 nm length scale.



Fig. 7. Calculated ligament yield strength (a) and modulus (b) as a function of ligament diameter. Also included are data obtained by microcompression test on Au pillars

The high yield strength of the ligaments of np-Au is consistent with recent nanomechanical measurements performed on submicron Au columns [41, 45, 46] and nanowires.[47] Both of these test specimens closely resemble the ligaments in foams, and mechanical tests reveal the general trend that "smaller is stronger". For example, Geer and Nix [45, 46] reported that the yield strength of submicron Au columns fabricated by focused ion beam micromachining approaches the theoretical yield strength of Au as the column diameter decreases to a few hundred nanometer. Specifically the yield strength data reported by Volkert and Lilleodden [41] are in excellent agreement with the size dependence observed for nanoporous Au: the yield strength of submicron Au columns follows the power law d^n , where d is the column diameter and n is 0.6. Figure 7a suggets that this size dependence continues to be valid down to 10 nm, the smallest ligament size which has been tested so far.

The size dependence of the yield strength observed in column microcompression tests has been explained by "dislocation starvation", that is the absence of efficient, easy-to-activate dislocation sources in sub-micron samples due to the presence of free surfaces. The argument goes along the following line: The smaller the sample volume (column/ligament), the smaller the dislocation source which can still be accommodated, the higher the stresses which are required to initiate yield. In this context, np Au can be envisioned as a three-dimensional network of defect-free, ultra-high strength Au nanowires.[37] Length-scale effects in plasticity can also be studied theoretically using molecular dynamics (MD) simulations.[48, 49] Preliminary molecular dynamics (MD) results show indeed that it is difficult to incorporate stable dislocation sources (such as a Frank-Read source) in nm-sized ligaments. These simulations also reveal that plastic deformation of nm-sized Au columns is still dislocation-mediated, and that these dislocations nucleate in the vicinity of step edges on free surfaces at stress levels close to the theoretical strength of the material (Figure 8).[49] Dislocation-mediated plasticity of nanometer-sized ligaments in nanoporous Au has recently also been observed experimentally using an in-situ transmission electron microscope nanoindentation technique.[50]

Additional factors which potentially could contribute to the higherthan-predicted strength are: testing method, densification, and grain size. For example, nanoindentation hardness and strength data obtained from fully dense materials show frequently higher values than those obtained by macroscopic tests, which is commonly attributed to the so-called "indentation size effect". We discard this possibility as the strength of nanoporous Au has been tested by a variety of different testing methods and generally good agreement has been found. Specifically, the micro-compression tests on nanoporous Au performed by Volkert et al.[36] have shown that the measured strength is independent of the test volume, consistent with the idea that the size effects in nanoporus Au are dominated by the ligament/pore dimensions and not by the sample size. Similarly, densification effects can be ruled out as the increase of strength with decreasing ligament size was observed for a fixed initial foam density. Finally, the grain structure of the ligaments or the lack thereof is still a subject of debate and is beyond the scope of this discussion [9]. However, even if we assume that the ligaments develop a nanocrystalline grain structure during dealloying, this would still not account for the high strength found experimentally since the yield strength of nanocrystalline Au [51, 52] is only 4 times higher than that of coarse-grained material.

The elastic properties of nanoporous Au have attracted less interest, and consequently there are fewer data available which, in addition, appear to be more scattered (Fig. 6b and Fig.7b). Most studies report Young's modulus values in the 5 to 13 GPa range consistent with the predictions



Fig. 8. Mechanical response of nanoscale Au pillars under compressive loading studied my MD. The displayed data were obtained from a 20 nm by 40 nm Au pillar compressed at 0K: a) Compressive stress-strain curve demonstrating the high yield strength of nanoscale Au ligaments; b) Nucleation of partial dislocations near the step edges revealing dislocation-mediated plasticity; c) Final state after 10% compression. The MD results were provided by courtesy of Dr. L. A. Zepeda-Ruiz and Dr. B. Sadigh,, LLNL

made by Eqn. 2 if one uses the bulk modulus of Au (~80 GPa) and relative densities ranging from 0.25 to 0.4. An exception to this is the recent study by Mathur and Erlenbacher [40] who reported a 4-fold increase in the Young's modulus, from ~10 GPa to ~ 40 GPa, as the ligament diameter decreases from >12 nm to 3 nm. The narrow range of most of the available data seems to indicate that there are little or no size effects in the elastic

properties. In principle, the high surface-to-volume ratio of the nanoscale ligaments in nanoporous Au could give rise to a size effect in the elastic properties: One can think of the ligaments as core-shell structures, where the core has bulk-like properties, and the shell exhibits elastic properties reflecting the reduced coordination number of surface atoms.[53] Depending on the actual electron redistribution caused by reduced coordination, the surface can become either softer or stiffer. Recent theoretical studies on Cu [54] showed that the effect of free surfaces on elasticity depends also on crystal orientation. However, even in the extreme case of a 2-layer system, the Young's modulus did not change by more than 50%.

Mathur and Erlenbacher [40] attributed the increased stiffness of ultrafine nanoporous Au to a combination of surface stress, density increase during dealloying due to shrinkage, and a higher bending stiffness of smaller ligaments. However, the 'smaller-is-stiffer' trend could also be caused by an increased level of residual Ag in sub-10-nm material. The preparation of this ultra-fine material requires dealloving conditions which strongly suppress surface diffusion. Experimentally, this can be achieved by using either dealloying potentials close to the Au oxidation potential,[55] or by performing the dealloying process at low temperatures.[20] Both methods have been shown to increase the amount of residual Ag which affects both the relative density and the elastic properties of the material. Unfortunately, many studies do not report the residual silver content, thus making the comparison from study to study more difficult. The effect of residual Ag on the elastic properties of nanoporous Au has recently been studied by Doucette et al.[56], who found that Ag doping generally increases the Young's modulus of nanoporous Au.

As mentioned above, one can think of nanoporous Au as a 3D network of Au nanowires. Thus it is instructive to compare the data discussed above with the literature on Au nanowires. Wu et al.[47] studied mechanical properties of Au nanowires ranging from 40 nm to 250 nm in diameter, and reported a Young's modulus of ~70 GPa, independent of the nanowire diameter and close to the value of bulk gold. Similar observations, namely a bulk-like behavior, have been reported for submicron Au columns.[41] The mechanical properties of sub-10-nm Au nanowires and pillars have been the subject of several molecular dynamics studies. Generally it was observed that the Young's modulus is only weakly dependent on the wire/pillar diameter (for wires which do not undergo a phase transformation [53]), and close to the value of bulk gold.[48, 57] Furthermore, it has been shown that the surface stress in these ultra-high surface-to-volume ratio systems mainly affects the strength by creating a compressive stress state in the wire/pillar core. In conclusion, most data presently available do not support the idea of a pronounced size effect in the elastic properties of nanoporous Au.

Fracture behavior

As discussed above, nanoporous Au has unique mechanical properties under compressive loading conditions where it combines high strength with high porosity. On the other hand, the material is notoriously brittle which severely limits its usefulness in terms of applications.[18, 58] Actually, the brittleness of nanoporous Au is the reason why scientists started to study the mechanical behavior of nanoporous Au in the first place: Ag-Au alloys were used to study stress corrosion cracking, that is, brittle failure of otherwise ductile materials in a corrosive environment.[59-61] These studies demonstrated that the formation of a thin surface layer of nanoporous gold is responsible for crack initiation and brittle failure of the uncorroded portion of the sample. Given the fact that Au is the most malleable metal, this brittle behavior is surprising. The questions which immediately arise in this context are: What causes the macroscopic brittleness of np-Au? Is the normal dislocation-mediated plasticity suppressed in nanoscale Au ligaments, or is the brittleness simply a consequence of the macroscopic morphology? These are the questions which will be addressed in the following.

The brittleness generally seems to increase with increasing Ag content of the Ag-Au master alloy, at least if dealloying is performed under free corrosion conditions: For example, samples made from Ag₇₀Au₃₀ alloys tend to be fairly robust, whereas samples made from Ag₈₀Au₂₀ alloys are generally more fragile. This trend seems to correlate with shrinkage and the buildup of tensile stress during dealloving which can induce crack formation.[8] In this context, it is interesting to note that thin-films and nanowires can accommodate this tensile stress better than macrocopic 3D samples as they are less constraint with regard to shrinkage: For example, nanoporous Au nanowires have been successfully prepared from Ag₈₂Au₁₈ alloys,[5] whereas a 3D sample prepared from such Ag-rich alloys would typically disintegrate during dealloying due to extensive cracking. The key to crack free material is to avoiding dealloying conditions which lead to extensive buildup of tensile stress. Indeed, fracture-resistant nonporous Au can be prepared by using dealloying conditions which promote stress relaxation, i.e. at elevated temperatures and lower dealloying potentials.[55]

As described above, brittle failure of nanoporous Au is observed under tensile loading conditions. Microstructural characterization of the fracture surfaces reveals that nanoporous Au fails by a combination of intra- and



Fig. 9. Fracture appearance of nanoporous Au of both intragranular (a) and intergranular regions (b). The inset shows the same region at higher magnification, and reveals the ductile nature of the fracture

intergranular fracture modes [58]: Intergranular fracture, where the crack follows the grain structure of the original AgAu master allow, reveals itself by the characteristic Rock candy morphology of the fracture surface, whereas intragranular fracture gives rise to smooth and featureless regions. On a microscopic level, however, characteristic necking features reveal ductile failure due to overloading of individual ligaments. In particular regions of intragranular fracture exhibit a high density of disrupted ligaments (Fig. 9). Intergranular fracture surfaces, on the other hand, exhibit a very smooth morphology with only a few disrupted ligaments. This difference can be explained by the presence of extended two-dimensional void-like defects which can be observed along the original grain boundaries of the master alloy. The formation of these defects can be explained by Ag enrichment at the grain boundaries which leads to the development of a reduced density material during dealloying. Indeed, Ag surface segregation during annealing has been reported for the Ag-Au system.[62] The fracture mode described here - brittle on a macroscopic length scale, but microscopically ductile – is not a unique feature of nanoporous gold, but has

recently even been observed for glass which is the common example for brittle failure.[63]

The two-dimensional void-like defects described in the previous paragraph presumably act as crack nucleation sites due to local stress enhancement (Fig 10). Ligaments connecting the regions on opposite sides of a defect experience the highest stress fields and are the first to fail. Once an unstable crack is formed, the crack propagates along the 2D defects until intersecting with another 2D defect at an oblique angle, where the fracture may or may not switch from intergranular to intragranular (see Fig. 9).



Fig. 10. Crack propagation along 2D defects, which are formed during dealloying along the grain boundaries of the original AuAg alloy. The crack (c) propagates from the right to the left along a defect. The remnant of a second grain boundary (gb) can be seen in the upper right Insert: A higher magnification image of the crack tip (ct) region reveals the void-like character of the 2D defects

The microscopic ductility of nanoporous Au is particularly obvious in the vicinity of crack tips, where highly strained ligaments still bridging the crack can be found (Fig 11). These ligaments show pronounced necking, and their elongation suggests strain values exceeding 100%. This microscopic ductility is also observed in molecular dynamics simulations on defect-free nanoscale Au columns under tensile loading (Fig 11). Here, the elongation to failure is in the order of 100%, consistent with the finding of highly strained ligaments near crack tips. The microscopic ductility is a remarkable result in the context of the macroscopic brittleness of np-Au, but is consistent with the fact that Au is the most malleable metal. This immediately raises the question of what causes the macroscopic brittleness of np-Au. A qualitative answer can be found by applying a random fuse network model [64, 65]: According to this model "brittle" failure can be expected for a sufficiently narrow ligament-strength distribution, regardless if the ligaments fail microscopically in a ductile or in a brittle manner. In the limit of a narrow ligament-strength distribution, rupture of the weakest ligament initiates the catastrophic failure of the network structure by overloading adjacent ligaments. The unstable crack then propagates quickly through the bulk of the material following the path of least resistance. This explanation is consistent with the narrow pore size/ ligament width distribution of np-Au observed experimentally, which implies uniform failure strength. The overall strength of a randomly fused network is determined by the largest "critical" defect; that is, the defect that causes the highest stress enhancement at its edge. In the case of nanoporous Au, the two-dimensional void-like defects formed during dealloying along the grain boundaries of the AgAu master alloy serve as crack nucleation sites by concentrating the stress on adjacent ligaments. Thus, instead of plastic deformation of the whole sample, the failure of a few ligaments triggers the brittle fracture of the network. This conclusion may be used to improve the mechanical properties of nanoporous Au by introducing a broader ligament strength distribution and by reducing the number and size of defects.



Fig. 11. Both SEM micrographs (left) and MD simulations (right) reveal the ductile failure behavior of nanoscale Au ligaments under tensile loading. The Au pillar used in the simulation is 5 nm by 10 nm, and snapshots of the configuration were taken at 0%, 25%, 50%, 100%, 125% and 150% strain. The MD results were provided by courtesy of L.A. Zepeda-Ruiz, LLNL

1.4. Summary

In this chapter we have reviewed the mechanical behavior for nanoporous Au. In contrast to macroporous foams, the yield strength of nanoporous Au increases dramatically with decreasing feature size. Consequently, a nanoporous metal foam can be envisioned as a three-dimensional network of ultrahigh-strength nanowires, thus bringing together two seemingly conflicting properties: high strength and high porosity. This highly unusual combination of material properties opens a new door for engineering applications. The elastic properties, on the other hand, seem to be much less affected by the nanoscale morphology of the material and can be reasonably well described by the scaling relations derived from macroporous foams. Currently, the macroscopic brittleness of np-Au presents a major obstacle to applications. This brittleness seems to arise from the network structure rather than reflecting a microscopic brittleness, and thus could potentially be overcome, for example by introducing a broader ligament strength distribution and by eliminating two-dimensional defects. As progress is achieved in understanding the mechanics of nanoporous materials, further research must include different types of nanoporous metals in order to developed more general trends.

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