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Title: Movement Orientation Switching with the Eyes and Lower Limb in Parkinson Disease

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Word Count: 4066

Figures: 3

Tables: 1

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### 1 Abstract

Difficulty switching between motor programs is a proposed cause of motor blocks in Parkinson 2 disease (PD). Switching from one movement to another has been studied in the upper extremity 3 4 and during postural control tasks, but not yet in the eyes and lower limb in PD. The purpose of this study was to compare movement orientation switching ability between people with PD and 5 age-matched controls (CON) and to determine if switching ability is correlated between the eyes 6 and lower limb. Twenty-six persons with PD and 19 age-matched controls participated. 7 Movement orientation switching was studied in a seated position with the head fixed in a 8 chinrest. In response to a randomly generated tone, participants switched from a continuous 9 back-and-forth movement in either the horizontal or vertical orientation to the opposite 10 orientation as quickly as possible. Lower limb movements were performed with the great toe 11 pointing back and forth between targets positioned on a 45° angled floor platform. Eve 12 movements were back and forth between the same targets. Eye and lower limb switch time was 13 reduced in PD (p<0.01), but after normalizing switch time to movement velocity, no differences 14 existed between PD and CON. Eye and lower limb switch times were correlated in PD (r=0.513, 15 p<0.01) but not in CON. In PD, switch time and movement velocity of the lower limb, but not 16 the eyes, correlated with bradykinesia and postural instability/gait. Our results suggest that 17 individuals with PD experience movement switching deficits with both the eyes and lower limb, 18 perhaps driven by overall bradykinesia. 19 20 21

22 Keywords: Parkinson's disease, eye movements, basal ganglia

## 24 1. Introduction

Many persons with Parkinson disease (PD) experience bradykinesia and akinesia that 25 often lead to functional decline including decreased mobility, freezing of gait, and a higher risk 26 27 of fall-related injuries. According to the center-surround hypothesis, basal ganglia dysfunction in PD may lead to excessive inhibition of desired and undesired movements<sup>1</sup>, leading to 28 difficulty with selection and execution of the desired movement. This difficulty has been cited 29 as a mechanism underlying problems with changing from one motor program to another  $^{2-4}$ , with 30 extreme difficulties in switching motor programs perhaps contributing to the freezing 31 phenomenon<sup>5</sup>. As freezing of gait is quite often triggered by turning, we hypothesize that 32 difficulties in switching between motor patterns in order to change direction of movement may 33 underlie the turning difficulties noted in many individuals with PD. Such impairments related to 34 switching movement direction have been reported for upper extremity movements and postural 35 control tasks <sup>4,6,7</sup>. Pfann et al. <sup>7</sup> even noted pauses, perhaps analogous to the freezing of gait 36 sometimes triggered by turning, at the points of direction change during upper extremity 37 movements. Specific impairments related to changing directions have also been hypothesized to 38 contribute to difficulties with sit to stand movements in individuals with PD<sup>8</sup>. 39 When considering direction changes, particularly during locomotion, one should not 40

when considering direction changes, particularly during locomotion, one should not
overlook the role of eye movements. Saccadic eye movements play an important role in
locomotion as they provide a shift in gaze toward the direction of travel and initiate the top-down
rotation sequence characteristic of a normal turning pattern <sup>9-11</sup>. Saccadic eye movements,
however, are impaired in PD, as evidenced by a large body of evidence. Early work in persons
with PD showed prolonged fixation times, bradykinesia, and akinesia during rapid alternating
gaze shifts between two fixed targets <sup>12</sup>. Several more recent studies have demonstrated that

47 people with PD make slower and smaller voluntary saccadesthan control subjects <sup>13-15</sup>. The basal 48 ganglia (BG) circuitry may be particularly important for changing saccade direction <sup>16</sup>, and 49 saccade dysfunction is associated with turning difficulty in persons with PD <sup>17</sup>. During both 90 50 and 180 degree turns, the saccade initiating the turn is hypometric and displays altered timing 51 relative to turn onset when compared with healthy controls.

To our knowledge, deficits in ability to change movement directions of the eyes and 52 lower limbs have yet to be examined in the same individuals with PD. Therefore, the purpose of 53 this investigation was to confirm whether individuals with PD have difficulty switching between 54 two movement orientations with the eyes and lower limbs, and to determine if the ability to 55 switch movement orientation with the eyes is correlated with switching ability in the lower limb. 56 We hypothesized that deficits in the ability to change movement orientation with the eyes and 57 lower limbs would be noted in individuals with PD, and that the deficits in the eyes and limbs 58 would correlate with one another, indicating a similar amount of decline in orientation switch 59 ability across different body parts. Confirmation of our hypotheses would support an overlap 60 between oculomotor and lower limb control in the dysfunctional BG and provide important 61 insights into the nature of eye and limb control in PD. 62

63 **2. Methods** 

### 64 2.1 Participants

Twenty-six individuals with idiopathic PD (17 men, 9 women; age = 70.2 ± 10.5; PD
duration 8.4 ± 6.0 years, Hoehn & Yahr stage = 2.3 ± 0.4; MDS-UPDRS III score = 41.0 ± 11.1)
and 19 age-and gender-matched controls (11 men, 8 women; age = 67.7 ± 10.6 years)
participated. Sample size was based on a-priori power analysis using switch time pilot data; 20
subjects per group would provide 87% power to detect a 0.7 effect size using a two-tailed, 2-way

ANOVA (p = 0.05). Individuals with PD were recruited from Washington University School of 70 Medicine's (WUSM) Movement Disorders Center. Controls were recruited from the Volunteers 71 for Health Database, posted flyers, and other WUSM volunteer databases. All subjects met the 72 73 following inclusion criteria: aged 30 years or older, normal central (except for PD in the PD group) and peripheral neurological function, able to stand independently for at least 30 minutes 74 and walk independently without an assistive device, no history of vestibular disease and no 75 evidence or history of dementia. Exclusionary criteria included: serious medical condition other 76 than PD, use of neuroleptic or other dopamine-blocking drug, use of drug that might affect 77 balance such as benzodiazepines, evidence of abnormality on brain imaging (previously done for 78 clinical evaluations-not part of this research), history or evidence of other neurological deficit, 79 and history or evidence of orthopedic, muscular, or psychological problem that may affect task 80 performance. Additionally, participants with PD were included based on a diagnosis of "definite 81 PD" by a board certified neurologist, as previously described by Racette et al.<sup>18</sup> based upon 82 established criteria<sup>19,20</sup> and were excluded if they had received surgical management of PD (e.g. 83 84 deep brain stimulation). All subjects gave informed consent to perform experimental procedures approved by the Human Research Protection Office at WUSM. 85

86 **2.2 Experimental procedures** 

All procedures were performed in the Locomotor Control Laboratory at WUSM.
Participants with PD were tested OFF medication, i.e. after a 12-hour withdrawal of all antiParkinson medications. Before testing procedures commenced, the Movement Disorder Society
Unified Parkinson's Disease Rating Scale (MDS-UPDRS) Motor Subscale III was administered
according to Goetz et al. <sup>21</sup> by a trained rater. The MDS-UPDRS-III is a measure of severity of
PD motor symptoms, as well as physical disability, and includes measures of rigidity, gait,

tremor, hand/arm and leg movements (bradykinesia), speech, and facial expressions. The
modified Hoehn and Yahr scale was used to evaluate disease severity in PD<sup>22</sup>. FOG was
assessed using the Freezing of Gait Questionnaire (FOG-Q)<sup>23</sup>, with total FOG-Q score
representing overall FOG severity, and freezers identified as those who reported freezing of gait
at least once per week on item three or the questionnaire.

During the protocol, each participant performed eye and lower limb movement tasks 98 while in a seated position. Lower extremity tasks were performed with the dominant limb. For 99 all movement tasks, four white targets were placed on a black angled platform (45° relative to the 100 floor) located on the floor in front of the subject. Targets were positioned 20 centimeters apart 101 such that eye movements between targets would be approximately 25 degrees (Figure 1). Each 102 subject was seated with his head resting in a chinrest to minimize head movement and angled 103 104 downward such that the platform was positioned in the center of the visual field. The platform was centered in front of the subject at a distance that allowed for comfortable movement of the 105 lower limb. To investigate the ability to switch movement orientation (switch task), participants 106 107 began the task by moving either their eyes or lower limb (pointing with the big toe) back and forth as quickly as possible between two targets (either horizontally or vertically). Upon hearing 108 an auditory tone, participants were instructed to switch movement orientation as quickly as 109 possible and continue moving back and forth in the new orientation. Multiple orientation 110 switches, including both horizontal-to-vertical (HV) and vertical-to-horizontal (VH) switches, 111 were performed at random times during each trial with 4-6 orientation switches per 30 second 112 trial. Auditory cues were triggered by the first author by pressing a button which sounded the 113 signal. Throughout each trial, the interval between switches was random as that the tester did not 114

time the interval between switch cues and made an effort to vary the time interval from switch to switch.

To control for differences in reaction time between PD and CON, simple reaction times 117 (RT) of the lower limb and eyes were tested. Each participant began with eyes fixated or great 118 toe positioned on a target centered between the 4 peripheral targets used for the switch task. 119 Upon hearing a tone, the participant reacted as quickly as possible to move either left, right, up, 120 or down, as instructed prior to each trial. To control for differences in movement velocity 121 122 between PD and CON, participants also performed three 10 second trials of back and forth movements of the eyes or lower limb, moving as quickly as possible between the horizontal 123 targets without switching orientations so that average movement velocity could be determined. 124 For all tasks, participants were given the opportunity to practice the task and data collection 125 126 commenced when the participant was comfortable performing the task.

#### 127 **2.3 Data collection and processing**

Lower limb movements were captured using an eight camera, passive marker, 3-128 129 dimensional, high-resolution motion capture system sampling at 100 Hz in Cortex software (Motion Analysis Corporation, Santa Rosa, CA). One retro-reflective marker was positioned at 130 the base of the great toe. The motion capture system was calibrated both statically (calibration 131 frame) and dynamically (wand) prior to each data collection session. Ocuolmotor data were 132 captured using a head-mounted infrared binocular eye tracking system (Applied Sciences 133 Laboratory, Bedford, MA) and electrooculography (EOG). Oculomotor data were captured 134 synchronously at 1000Hz on the same PC workstation with kinematic data in Cortex software. 135 The infrared eye tracking system was calibrated for each participant using a two step process. 136 137 First, a nine-point relative points methods was used to calibrate the eye tracking system. Then,

allow conversion of analog data (millivolts) into angle data (degrees). 139 Lower limb marker data and analog data were filtered using 4th order low-pass 140 141 Butterworth filters. Marker data were filtered in Cortex with a cut-off frequency of 6 Hz while analog data were filtered in MotionMonitor (Innsport, Chicago, IL) with a cut-off frequency of 142 20 Hz. A global coordinate system was defined in MotionMonitor with the positive X-axis 143 pointing anteriorly, positive Y-axis pointing to the left and positive Z-axis pointing upward 144 vertically. Toe marker kinematic data and filtered analog data were exported for further 145 processing in custom written MATLAB software (The Mathworks, Inc, Natick, MA). 146 For the orientation switch task, switch time was defined as the time interval between the 147 auditory tone and the beginning of first full amplitude movement in the new orientation. As each 148 149 trial contained multiple VH and HV switches, VH and HV switches were measured separately and an average switch time was determined for each switch orientation. For the RT tasks, RT 150 was defined as the time interval between auditory tone and movement onset (lower limb 151 152 movement exceeding 5 mm from origin and eye movements exceeding 0.5 degrees from origin). For the movement velocity task, movement velocity was calculated as the number of back and 153 forth cycles completed during a measured time period multiplied by the average movement 154 amplitude across all of the cycles within the trail. Finally, to control for the effect of movement 155 velocity, switch times were normalized to movement velocity by multiplying the two measures. 156 Individual trials were excluded from analysis if artifacts in oculomotor data due to blinks, 157 prolonged closure of eyelids, or other factors precluded measurement. Remaining trials within a 158 condition were averaged to obtain a single data point for each subject for each task. 159 160 2.4 Data Analysis

participants performed saccades of known amplitudes in four directions (up, down, left, right) to

161	Independent Student's t-tests were used to compare between-group differences in
162	movement velocity, movement amplitude, and normalized switch time for both the eyes and
163	lower limb, and a bonferroni correction was used to control for multiple comparisons, bringing
164	the level of significance for the t-tests to p<0.0045. A mixed model was used to test the effect of
165	group, segment (eye vs. lower limb), and the group-segment interaction on switch time and RT.
166	Segment was treated as a repeated measure. Pearson's correlation coefficients were used to test
167	the correlation between eye and lower limb switch times as well as the correlation between
168	switch time and movement velocity. Spearman's rank order correlations were used to examine
169	correlations between movement parameters (amplitude, velocity, switch time) and FOG and the
170	MDS-UPDRS III. The criterion for statistical significance was set at p<0.05 for all analyses.
171	3. Results
172	Eye movements in the vertical plane could not be captured for a number of participants
173	(13 PD and 2 CON). Therefore, only movement tasks in the horizontal plane and VH orientation
174	switches are reported. Age did not differ between PD and CON (t = .799, $p = 0.429$ ), nor did RT
175	(F = 1.703, p = 0.199), although RT was slower in the lower limb (F = 28.343, p < 0.001).
176	Movement velocity was not statistically different between PD and CON for the eyes ( $t = 1.505$ , p
177	= 0.140), but was decreased in PD for the lower limb (t = $3.710$ , p = $0.001$ ). There was a
178	significant group effect for switch time (F = 20.99, p < 0.001), but neither the main effect of
179	segment nor the group-segment interaction were significant (F=2.386, $p = 0.130$ ; F = 0.143, $p = 0.143$ , p =
180	0.707, respectively). Although switch time was significantly different between groups,
181	normalized switch time did not differ significantly between groups for the eyes ( $t = 1.683$ , $p =$
182	0.100) or lower limb (t = 1.138, p = 0.261). During the movement velocity task, average lower
183	limb and eye movement amplitudes closely approximated the expected values based on target

placement (20 cm/ 25 degrees apart), and there were no group differences for the eyes (t = 0.453, p = 0.653) or lower limb (t = 1.949, p = 0.058). Eye and lower limb performance data are displayed in Table 1.

Across all participants, switch times of the eyes and lower limb were significantly 187 correlated (r = 0.425, p = 0.004), but normalized switch times of the eyes and lower limb were 188 not significantly correlated (r = 0.257, p = 0.088). Within PD, eye and lower limb switch time 189 190 did not correlate significantly (r = 0.286, p = 0.186) but normalized switch times correlated significantly (r = 0.513, p = 0.007). Within CON, neither correlation was significant (switch 191 time, r = 0.089, p = 0.719; normalized switch time, r = -0.058, p = 0.812) (Figure 2). In PD, 192 FOG was correlated with lower limb velocity ( $\rho = -.483$ , p = 0.013), amplitude ( $\rho = -0.552$ , p =193 0.007), and switch time ( $\rho = 0.503$ , p = 0.009). Total MDS-UPDRS-III scores correlated with 194 lower limb switch time ( $\rho = 0.502$ , p=0.009), velocity ( $\rho = 0.551$ , p = 0.004), and amplitude ( $\rho =$ 195 -0.606, p = 0.001). MDS-UPDRS-III scores were also divided into sub-scores reflecting tremor 196 (items 3.15 - 3.18), rigidity (item 3.3), bradykinesia (items 3.4 - 3.8), and postural stability and 197 198 gait (PIGD, items 3.9 - 3.13). PIGD correlated with lower limb switch time ( $\rho = 0.558, 0.003$ ), velocity ( $\rho = -0.617$ , p = 0.001) and amplitude ( $\rho = -0.430$ , p = 0.032). Bradykinesia correlated 199 with lower limb switch time ( $\rho = 0.412$ , p = 0.036) and velocity ( $\rho = -0.493$ , p = 0.010). Eve 200 201 switch time and velocity did not correlate significantly with any of the MDS UPDRS III subscores. These correlations are shown in Figure 3. Finally, switch time and movement velocity 202 were significantly correlated in the eyes (r = -0.587, p < 0.001) and in the lower limb (r = -0.749, 203 p < 0.001) across all participants. 204 Comparing freezers and non-freezers. groups did not differ in terms of movement

205 Comparing freezers and non-freezers. groups did not differ in terms of movement 206 velocity (eye, t = 1.045, p = 0.306; lower limb, t = 1.134, p = 0.268) or amplitude (eye, t = 0.007,

p = 0.775, 10 wer mind, $t = 0.052$ , $p = 0.4057$ . The main effect of eye vs. 10 wer mind
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significant for RT (F = 21.248, p < 0.001) with RT being slower in the lower limb. Both the main

effect of group (F = 0.039, p = 0.845) and the interaction (F = 1.343, p = 0.258) were not

significant for RT. Switch time main effect of group (F = 1.081, p = 0.309), eye vs. lower limb

211 (F = 1.936, p = 0.177), and the interaction (F = 3.247, p = 0.084) were all non-significant.

#### 212 **4. Discussion**

This study sought to determine whether the ability to switch movement orientation with 213 the eyes and lower limbs is impaired in PD and whether orientation switch ability is similar 214 between the eyes and lower limbs. In summary, persons with PD took longer to switch 215 movement orientation with both the eyes and lower limb, and displayed a reduction in lower 216 limb movement velocity. When normalizing switch time to movement velocity, the significant 217 218 group effects of switch time were negated. Across both PD and CON, eve switch time correlated 219 significantly with lower limb switch time, and in persons with PD, FOG, UPDRS, PIGD, and bradykinesia correlated significantly with lower limb function, while oculomotor function did 220 221 not correlate with these measures. There were no differences between PD freezers and nonfreezers in terms of switch time, movement velocity, or movement amplitude 222

Our hypothesis was supported in that persons with PD required 37% and 41% more time to switch orientation with their eyes and lower limb, respectively, compared to controls. However, since eye and lower limb movement velocities were slower in PD compared with CON, we normalized orientation switch times to movement velocity. In doing so, we noted that normalized switch times were similar between PD and controls, indicating that if PD were to move at the same velocity as the controls, their orientation switch ability may be comparable for both the eyes and lower limbs. As hypothesized, normalized lower limb switch times explained 26% of the variance in normalized eye switch times in PD, but this relationship did not hold truefor controls.

Our finding of prolonged switch times in PD corroborates previous research. In the 232 upper extremity, Almeida et al.<sup>24</sup> observed delays in switching between two coordination 233 patterns in the upper extremity, while Plotnik et al.<sup>6</sup> showed that people with PD respond poorly 234 to movement modifications. To our knowledge, this is the first study to report such findings in 235 236 the lower extremity and eyes. Further, previous studies in the upper extremity did not account for movement velocity. Herein, we demonstrate that accounting for movement velocity negates 237 the group differences in orientation switch ability. Thus, observed deficits in the ability to 238 switch movement direction/orientation in our study and others, indicative of a deficit in motor 239 program switching, may be simply a function of global bradykinesia. Regardless, it is clear that 240 241 the overall time required to change from one movement paradigm to another in response to an external stimulus is greater in PD. This difficulty may contribute to FOG which is often 242 triggered by a change in movement, such as switching from straight walking to turning. The 243 244 modest delay in switching between simple motor programs observed in the present study may manifest in a much longer delay or freeze when the motor programs are more complicated (i.e. 245 gait). A delay in switching could also be a contributing factor in falls, as a delay in selecting and 246 executing the proper motor response to an unanticipated perturbation or change in body position 247 may not allow enough to time to catch oneself before a point of no return. Finally, our study 248 supports previous work showing deficits in oculomotor function in PD. Visual information plays 249 an important role in gait and people with PD show deficits in saccade performance that relate to 250 impaired turning performance <sup>17</sup> and may contribute to FOG and falls. 251

While the basal ganglia are often described as having distinct loops for oculomotor and 252 motor control, evidence suggests that the subthalamic nucleus (STN) may play key roles in the 253 control of both eye and limb movements, indicating overlap of the oculomotor and motor loops. 254 Some neurons within the STN respond to voluntary saccades as well as limb movements <sup>25</sup>. The 255 timing and characteristics of saccade-related potentials in STN suggest that these cells are 256 responsible for broad non-specific inhibitory output to inhibit unwanted motor programs, 257 whether for the eyes or the limbs <sup>26</sup>. Disruption of this inhibitory output from the STN could 258 account for impairments in voluntary saccades <sup>27</sup> and limb movements. Abnormal STN output 259 may also contribute to difficulty turning that can trigger FOG, as evidenced by the fact that STN 260 deep brain stimulation can alleviate off-period freezing<sup>28-30</sup>. The apparent overlap between 261 oculomotor and motor control in the basal ganglia provides a potential anatomical substrate 262 where a pathophysiological disruption could contribute to impaired eye and limb movements and 263 also to turning difficulties. Our data suggest that eye and lower limb switching are mildly 264 correlated, supporting the potential for overlap between oculomotor and lower limb control by 265 266 the basal ganglia and a global bradykinesia that appears to influence eye and limb movements similarly. In line with a center surround hypothesis<sup>1</sup>, the common bradykinesia of the eyes and 267 lower limbs may be due to over-activity of the subthalamic nucleus leading to excessive 268 inhibitory output from the basal ganglia. In support of a global bradykinetic cause for delays in 269 switching movement orientation in the tasks we studied, our global bradykinesia score obtained 270 from the MDS-UPDRS-III correlated with lower limb orientation switch times, as did the PIGD 271 score. 272

While we conclude that differences in switch time between PD and CON are driven bybradykinesia, it is important to consider alternative hypotheses. Since the switch task involved

reacting to an auditory stimulus, differences in switch times could be attributed to differences in 275 RT between PD and CON. However, RT did not differ between groups for either the lower limb 276 or eyes, thus RT is unlikely to have contributed to group differences in switch time. An 277 278 alternative hypothesis to our bradykinesia explanation is that PD suffer from a deficit in the ability to select and execute a new or different motor program, and that this deficit is at least 279 partially independent of bradykinesia. If this were the case, we would expect group differences in 280 switch time to remain even after controlling for movement velocity (normalized switch times), 281 indicated that bradykinesia does not fully explain the effect of group on switch time. However, 282 this was not the case as normalized switch times were very similar between PD and CON for 283 both the eyes and lower limb. Further support for our bradykinesia hypothesis is that movement 284 velocity and switch time were highly correlated in both the eyes and lower limb across all 285 286 subjects, and that there were no differences between freezers and non-freezers in the ability to switch movement orientation. 287

#### 288 4.1 Limitations

During the movement velocity and orientation switch tasks, participants were provided 289 with visual cues in the form of targets. A large body of existing literature supports the use of 290 various types of visual cueing strategies for improving movement in PD. Therefore, it is 291 possible that movement amplitude and switching ability were enhanced in PD by the presence of 292 targets. Additionally, the lower limb and eye movements required for the tasks herein were of 293 relatively small amplitude (20cm for the lower limb and 25 degrees for the eyes). Since the 294 performance of those with PD compared well with controls in terms of movement amplitude, it is 295 possible that the inter-target distance chosen was too small to elicit hypokinetic movement in 296 297 PD.

298 4.2 Conclusions and future directions

Switching between movement contexts is impaired in PD and affects not only upper and lower limb movements, but eye movements as well, and the severity of dysfunction is similar between eyes and lower limb. It appears that global bradykinesia may be a factor affecting switching ability in PD. Future work should explore movement switching ability of the lower limbs during more complex and functionally relevant tasks, such as during locomotion.

#### 304 Acknowledgements

We thank Marie McNeely and Ryan Duncan for assistance with data collection, Brian Morrell 305 for assistance with data processing, and Dr. Richard Abrams for assistance with project design 306 and pilot testing. This publication was made possible by NIH grant R01 HD056015, the Barnes 307 Jewish Hospital Foundation, and Grant Number UL1 RR024992 from the National Center for 308 309 Research Resources (NCRR), a component of the National Institutes of Health (NIH), and NIH 310 Roadmap for Medical Research. Its contents are solely the responsibility of the authors and do not necessarily represent the official view of NCRR or NIH. Additional support came from the 311 312 St. Louis Chapter of the American Parkinson Disease Association (APDA) and the APDA Advanced Center for PD Research at Washington University in St. Louis. 313 314 315 316 317 318

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## 403 FIGURES





Figure 1. Experimental set-up. (A) Participants were seated in a chair with their head positioned
in a chinrest to minimize head movement and with their head tilted downward. A binocular
head-mounted eye tracking device was secured to their head in this position. A black platform
was positioned on the floor in front of the subjects. The platform was angled 45 degrees to the
floor with round white targets positioned on the face of the platform. (B) Configuration of
targets for the orientation switch task. (C) Configuration of targets for the reaction time task.



**Figure 2.** Correlation between eye and lower limb switch times for CON (top) and PD (bottom).





Figure 3. Correlations of lower limb switch time (left column) and movement velocity (right
column) with MDS-UPDRS III, Bradykinesia, PIGD, and FOG in subject with PD only.

Measure	PD	(n)		Controls	(n)
Eye RT (sec)	$0.293 \pm 0.061$	26		$0.286 \pm 0.034$	18
Foot RT (sec)	$0.360 \pm 0.064$	26		$0.336 \pm 0.062$	19
Eye Velocity (degrees/sec)	$48.05 \pm 15.9$	26		54.84 ± 13.5	19
Foot Velocity (cm/sec)	$34.40 \pm 12.6$	25	t	$47.89 \pm 11.2$	19
Eye Amplitude (degrees)	$24.8 \pm 4.2$	26		$25.1 \pm 0.9$	19
Foot Amplitude (cm)	$18.5 \pm 0.01$	25		$19.3 \pm 0.01$	19
Eye Switch Time (sec)	$1.00 \pm 0.294$	26	Ť	$0.731 \pm 0.134$	19
Foot Switch Time (sec)	$1.11 \pm 0.366$	26	Ť	$0.789 \pm 0.126$	19
Normalized Eye Switch Time <sup>a</sup>	$45.25 \pm 12.42$	26		39.56 ± 9.26	19
Normalized Foot Switch Timeb	34.46 ± 7.34	26		36.96 ± 7.17	19

## Table 1. Eye and lower limb performance data.

Values are means ± standard deviations.

<sup>a,b</sup> Arbitrary units \* Significantly group effect, p < 0.05 † Significantly group effect, p < 0.01