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Physical properties and bioactivity of Aloe vera modified tricalcium silicate-based cement

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1 **Physical properties and bioactivity of Aloe vera modified tricalcium**
2 **silicate-based cement**

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9 **Running title:**

10 Physical properties of Aloe vera modified cement

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23 **Abstract**

24 **Objective:** This study compares the physical properties and bioactivity of tricalcium
25 silicate-based cement (Matreva MTA) modified with various concentrations of Aloe
26 vera (AV) solutions and Biodentine cement.

27 **Methods:** Sixty discs were prepared, and divided into 5 groups (12 discs each) based
28 on the estimated materials: group I: Biodentine, group II: Matreva MTA, group III:
29 Matreva MTA with 10% AV, group IV: Matreva MTA with 20% AV and group V:
30 Matreva MTA with 30% AV. The flow and setting time were assessed following ISO
31 standard 6876:2012 and **American Society for Testing and Materials** (ASTM)
32 standard C266-21, respectively. The in-vitro bioactivity was evaluated after 1, 14, and
33 28 days of immersion in Hank's balanced salt solution (HBSS) including pH, calcium
34 ion release, and apatite formation. All data were statistically analyzed.

35 **Results:** Increasing the AV concentration added to Matreva MTA from 0 to 30%
36 decreased the flow and setting time. Significant high mean pH and calcium ion release
37 values were observed for 20 and 30% AV-modified Matreva MTA cement at 14 and
38 28 days ($P \leq 0.05$). **Environmental scanning electron microscope/ energy-dispersive**
39 **X-ray spectroscopy (ESEM/EDX)** analysis confirmed calcium phosphate nucleation
40 on the surfaces of 20 and 30% AV-modified Matreva MTA cements after immersion
41 in HBSS.

42 **Conclusion:** Addition of 20 and 30% AV solutions to Matreva MTA reduced the
43 setting time and improved the handling characteristics as well as the in-vitro
44 bioactivity, resembling the qualities of Biodentine. Both AV-modified Matreva MTA
45 and Biodentine cements had extended alkalinizing activity and calcium ion release.

46 **Clinical relevance:** AV-modified Matreva MTA can be considered a promising
47 biomaterial for different endodontic applications.

48 **Keywords:**

49 Aloe vera, Bioactivity, Biodentine, Flow test, Matreva MTA, Setting time

50 **Introduction**

51 Mineral trioxide aggregate (MTA) has received considerable attention due to its
52 outstanding biocompatibility, sealing ability, and antibacterial qualities [1-5]. It was
53 first developed as a material for the repair of root perforations, but it is now utilized in
54 regenerative endodontic therapy, vital pulp therapy, and the management of dentine
55 hypersensitivity [6-9]. However, the practitioner is still faced with difficulties due to
56 its lengthy setting time, challenging handling characteristics, expensive material cost,
57 and discoloration potential [4,10].

58 Biodentine (Septodont, Saint Maur des Fosses, France), was recently introduced as a
59 new fast-setting biomaterial that is suggested for use as a dentine replacement in
60 similar applications as MTA [11-13]. The addition of setting accelerators and
61 softeners, as well as a new pre-dosed capsule formulation for use in a mixing device,
62 primarily improve the physical properties of biodentine, making it much more user-
63 friendly [14,15].

64 *Aloe vera* plant belonging to the *Liliaceae* family has been widely utilized in
65 pharmaceutical manufacturing due to its anti-inflammatory, antibacterial, antioxidant,
66 antiviral, antifungal, hypoglycemic, immune-modulating action, wound healing, and
67 regenerative properties [16,17]. *Aloe vera* powder contains more than 75
68 physiologically active and naturally occurring ingredients, including polysaccharides,
69 amino acids, vitamins, lipids, sterols, and minerals [16]. Most of the functional
70 activities associated with using *Aloe vera* plant are attributed to the polysaccharides

71 (such as Acemannan and glucomannan) [16,18]. *Aloe vera* has been used to treat
72 periodontal disease, angular cheilitis, aphthous ulcers, denture-related stomatitis,
73 and intracanal medication [16,19]. When used as a pulp dressing material, AV has
74 also proven to have anti-inflammatory and wound-healing properties [16,20,21].
75 Therefore, this study evaluated the physical properties and bioactivity of tricalcium
76 silicate-based cement (Matreva MTA) modified with an AV-based solution in
77 comparison with Biodentine for various endodontic applications.

78 **Materials and methods**

79 The materials utilized in the current study are shown in table 1.

80 **Cement preparation and grouping of specimens**

81 Matreva powder was mixed with either pure distilled water (0% AV) or with 10, 20,
82 or 30% AV-modified distilled water at a powder/ liquid ratio of 3:1 by weight as
83 recommended by the manufacturer. Biodentine was also mixed using the
84 manufacturer's guidelines. The fresh pastes were packed into a split Teflon mold with
85 a 10 ± 0.1 mm diameter and 2 ± 0.1 mm thickness on a clean glass slide. The top surface
86 of the mold was then covered with a celluloid strip and a glass slide and left
87 undisturbed until hardened (set). Sixty disc specimens were prepared for the five
88 groups (12 discs each): group I: Biodentine, group II: Matreva MTA, group III
89 Matreva MTA 10% AV, group IV: Matreva MTA 20% AV and group V: Matreva
90 MTA 30% AV.

91 **Assessment of the physical properties**

92 ***Flow test***

93 Each group's flow (n=6) was established in accordance with ISO standard 6876 [22].
94 After mixing, 50 μ L (0.05 mL) of each substance was immediately placed onto a
95 glass slab (40x40x5 mm). A second glass slab (20 g weight) was placed on the

96 material with 100 gm weight on top. A digital caliper was then used to measure the
97 maximum and minimum diameters of the formed disc and the mean diameter was
98 considered as a measurement of the flow.

99 *Setting time*

100 The initial setting time and final setting time were measured (n=6 discs) by Gilmore
101 needles in accordance with the ASTM standard C266-21 [23]. The initial Gilmore tip
102 (113.4 g weight and 2.12 mm diameter) and the final Gilmore tip (453.6 g weight and
103 1.06 mm diameter) were utilized on the cement paste during the setting.

104 **Bioactivity testing**

105 Set cement discs from each investigated group (n=6 discs) were submerged in 10 mL
106 of HBSS (Lonza, Walkersville, MD, USA) in a sealed 50 mL sterile polypropylene
107 tube and kept in an incubator (Titanox, TITANOX art, A3-213-400I Co., Italy) at
108 37°C. The solution was collected for pH and calcium ion evaluation after 1, 14, and
109 28 days.

110 *Alkalizing activity and calcium ion release*

111 The pH was quantified using a pH meter (HI98103, Hanna Instruments Inc., USA).
112 Three readings were average for each sample. Calcium ion analysis was analyzed
113 using an inductively coupled plasma mass spectroscopy (ICP/MS) (Agilent 7700,
114 Agilent Technologies, Germany).

115 *Apatite-forming ability*

116 The discs were collected after 1, 14, and 28 days. The specimens' surfaces were tested
117 without any modification or coating using an ESEM attached to EDX Unit (Inspect,
118 FEI Company, Netherlands) at 2000 and 5000 X. Elemental analysis using EDX was
119 utilized to estimate the surface calcium-to-phosphorus (Ca/P) atomic ratios. The discs
120 were returned into a new 10 mL of HBSS after 1 and 14 days and kept in the

121 incubator until the following interval. The discs were scrapped with a sterile spatula to
122 be examined by X-ray Diffraction (XRD) and Fourier-Transform Infrared (FTIR)
123 spectroscopy after storage in the Hank's balanced salt solution (HBSS) for 28 days.

124 **Statistical analysis**

125 Data were analyzed using one-way ANOVA (setting time and flow test), and two-way
126 ANOVA (pH and ion release test), followed by Tukey's post hoc test. The
127 significance threshold was set at $P \leq 0.05$ for all tests. Statistical analysis was
128 performed using the R statistical analysis software for Windows, version 4.0.3 (R
129 Foundation for Statistical Computing, Vienna, Austria).

130 **Results**

131 **Physical properties of the tested materials**

132 *Flow and setting time findings*

133 Group II had the highest mean flow value while group V showed the lowest mean
134 value (Table 2). There was a statistically significant difference among groups II and
135 III ($P < 0.05$) while no statistically significant difference was noted among groups I, IV
136 and V ($P > 0.05$).

137 Regarding the initial setting time, group II showed the highest mean value while
138 group I showed the lowest mean value. The pairwise comparison revealed a
139 significant difference among all groups ($P < 0.05$) except for groups I and V, where no
140 significant difference was found ($P > 0.05$).

141 For the final setting time, group II showed the highest mean value while group I
142 showed the lowest value. Pairwise comparison showed a significant difference among
143 all groups ($P < 0.001$).

144 **Bioactivity of the tested materials**

145 *Alkalizing activity and calcium ion release results*

146 The tested material, time, and their interaction had a significant effect on pH and Ca⁺²
147 ion release values (P<0.001).

148 Regarding the pH measurements (Figure 1a), day 1 showed the highest mean value
149 followed by day 14 while day 28 showed the lowest mean value in all groups with a
150 significant difference among the different time periods (P<0.001).

151 As for calcium ion release (Figure 1b), the highest mean value was observed on day 1
152 followed by day 14 while day 28 showed the lowest mean value in group I (P<0.001).

153 On the other hand, in groups II, III, IV, and V, day 28 showed the highest mean value
154 followed by day 14 while day 1 showed the lowest mean value with a significant
155 difference among the different time periods (P<0.001).

156 *Apatite forming ability*

157 *ESEM and EDX findings after immersion in HBSS*

158 The results of ESEM of the Biodentine stored in HBSS for different periods showed
159 the gradual formation of superficial spherules on the Biodentine surface. The amount
160 of surface layer increased with increasing the immersion time from 1 d to 28 d. The
161 EDX elemental analysis showed peaks denoting the different reaction phases present
162 in the set cement and calcium phosphate layer with decreasing calcium/phosphorus
163 ratio over time. These calcium phosphate crystals suggested the creation of an apatite
164 layer (Figure 2). Increasing the soaking time in HBSS revealed the disappearance of
165 zirconium peaks and a decrease in the intensity of silica components while Mg
166 element from HBSS became detectable.

167 When Matreva MTA and AV-modified Matreva MTA groups were stored in HBSS
168 for different time intervals; ESEM analysis revealed that superficial irregularly
169 distributed Ca and P precipitates were gradually forming on the surface of the
170 Matreva MTA (Figures 3-6). This surface layer grew when the immersion period was

171 extended from 1 to 28 d. In comparison to the unmodified Matreva MTA during the
172 same period, the calcium phosphate that was generated on the surface of the AV-
173 modified groups was much denser. The calcium phosphate layer and other reaction
174 phases were visible as peaks in the set cement's EDX measurement, and the
175 calcium/phosphorus ratio decreased with time.

176 *XRD findings after immersion in HBSS*

177 XRD analysis of the hydrated Biodentine revealed peaks denoting calcium carbonate
178 (calcite), and calcium hydroxide (portlandite) with obliteration of the tricalcium
179 silicate peaks at the range of 32 to 40°. XRD spectral analysis of the hydrated Matreva
180 MTA revealed peaks denoting calcium carbonate (calcite) at 30° and calcium
181 hydroxide (portlandite) at 17°. According to the results of XRD, the calcium
182 hydroxide peak increased after immersion in HBSS for 28 d. However, its peak
183 slightly decreased with an increasing ratio of AV from 0 to 30% (Figure 7a).

184 *FTIR findings after immersion in HBSS*

185 After immersion in HBSS, FTIR analysis of Biodentine revealed distinct split peaks at
186 ~500, 620, and 820 cm^{-1} . These peaks were consistent with apatite development
187 representing apatite precursors, such as octa-calcium phosphate. A broad band of CSH
188 within the 800–1000 cm^{-1} range was observed. Matreva MTA's FTIR absorbance
189 spectra showed intensified bands of portlandite, CSH phase, and an apatite deposit. In
190 addition, the bands of calcium carbonate (calcite, aragonite, vaterite), belite, and alite
191 were still observable. A high band at ~950 cm^{-1} was assigned to PO_4^{3-} from apatite.
192 The CO_3^{2-} stretching from calcite (CaCO_3) and carbonated apatite was visible at
193 ~1400 cm^{-1} . Bands at ~1070 and 860 cm^{-1} were also assigned to PO_4^{3-} denoting
194 symmetric stretching from apatite (Figure 7b).

195 **Discussion**

196 The current study evaluated the impact of AV solutions for the modification of
197 tricalcium silicate-based cement (Matreva MTA), as a lower-cost alternative to
198 Biodentine cement. Biodentine is known to have good physical properties, handling
199 characteristics, biocompatibility, and wide clinical applications [13,24].

200 The flow and setting time were assessed following ISO standard 6876:2012 and
201 ASTM standard C266-21, respectively. No significant differences in flow were found
202 among Biodentine, 20% AV, and 30 % AV-modified groups. The modification of
203 Matreva MTA with AV slightly reduced the flow and imparted the material with a
204 putty-like consistency which may favor easier clinical manipulation. This was in
205 accordance with a previous study by Borges et al. who investigated the
206 physicochemical features of MTA and Portland cement associated with a 2% glycolic
207 solution including *Aloe vera* [25]. Another study examined the physicochemical,
208 antibacterial, and biological effects of white MTA combined with aqueous and
209 propylene glycol extracts of *Arctium lappa* L. and *Casearia sylvestris* SW. The
210 findings indicated that propylene glycol-mixed cement had long initial and final
211 setting times and increased flow [26].

212 Regarding the setting time, the findings showed that the AV-modified Matreva MTA
213 groups had a shorter setting time (initial and final) compared with the unmodified
214 Matreva MTA. The mean initial setting time reduced from ~39.21 to ~17.83 min, and
215 the mean final setting time decreased from ~98.67 to ~58.83 min, respectively, as the
216 concentration of AV solution increased from 10 to 30%. While the initial setting times
217 for the AV-modified Matreva MTA groups and Biodentine were comparable. A short
218 setting time, like that obtained in the present study for 30 % AV-modified Matreva
219 MTA is advantageous as it allows placement of the final restoration at the same visit.
220 The ability of AV to create aggregated lumps of hydrophilic colloids may have

221 accelerated the final set by facilitating the transport of ions and water into the calcium
222 silicate [27]. Fortunately, this was not associated with a compromise in its
223 workability.

224 The release of calcium and hydroxide ions from endodontic and pulp capping
225 materials is considered a key factor for their success [28]. Calcium and hydroxide ions
226 stimulate alkaline phosphatase enzymes and the differentiation of hard tissue-forming
227 cells for mineralization/ bioactivity [29]. ICP-MS was used to measure calcium ion
228 release because it is an advanced and accurate method analyzing of leached ions in
229 media in trace levels despite the liquid pH [30].

230 Both Biodentine and Matreva MTA groups released calcium ions and induced
231 alkalization (elevated pH). Biodentine initially released a significantly higher amount
232 of calcium ions (253 ppm) after one day and produced a strong alkalization which
233 significantly decreased with time in contrast to unmodified Matreva MTA which
234 released the lowest calcium ion value (9.71 ppm). This may be due to the high
235 solubility and fast hydration reaction of Biodentine in the early few hours after
236 preparation. These findings are in accordance with earlier results [31]. This contrasted
237 with prior research by Kumari et al. which found that MTA released considerably
238 more Ca ions than Biodentine during the experiment but that difference increased and
239 became greater after 28 d [32].

240 The pH measurements of all groups gradually decreased as the storage time increased
241 from 1 to 28 d. This agreed with a previous study by Dsouza et al. [33]. However,
242 calcium ion release significantly increased with increasing the storage time except for
243 Biodentine, which decreased with time. These ions are then released to the
244 surrounding medium where the hydroxyl ions increase pH which could induce an
245 antibacterial effect and favors apatite precipitation [31,34]

246 The ion release process depends upon several factors like nature, size, porosity,
247 density, and distribution of the mineral particles [3,34]. Therefore, porosity may
248 increase with the increase in water sorption of AV-modified Matreva MTA providing
249 a more bio-interactive surface for the calcium and hydroxyl ions release. This could
250 explain the prolonged alkaline pH and the large, sustained calcium ions release
251 observed in the present study.

252 In the current work, HBSS was used to simulate the ionic concentrations of the human
253 blood plasma and mimic the biological fluids (blood, exudates, plasma, and dentinal
254 fluid) as a source of phosphate ions to trigger the precipitation of calcium phosphate
255 (apatite) on the surface of calcium leaching materials [35]. Thus, the experimental
256 samples were soaked in HBSS for 28 d for the same specimen. This allowed a better
257 correlation between the resultant data and monitoring of the changes that occur over
258 time.

259 Different kinds of cements were evaluated for their *in-vitro* bioactivity using the
260 ESEM/EDX, XRD, and FTIR analyses [3,13]. The utilization of the ESEM analysis
261 was to avoid surface coating of the specimen before imaging, to prevent surface
262 alterations, and to allow the usage of the same specimen throughout time intervals.

263 All materials formed superficial, spherical crystalline precipitates after being
264 submerged in HBSS. These precipitates increased in amount and thickness from 1 to
265 28 d. These precipitates contained Ca and P as their main constituents, suggesting the
266 formation of an apatite layer. EDX elemental analysis showed other elements in
267 addition to the calcium phosphate layer. The Ca/P ratio decreased with increasing
268 storage times as phosphorus peaks increased with increasing immersion time. ESEM
269 assessment showed that AV-modified Matreva MTA produced a denser and thicker
270 surface layer than the unmodified Matreva MTA cement at all-time intervals. The

271 higher AV concentration also increased the precipitated calcium phosphate layer,
272 suggesting the better apatite-forming ability of Matreva MTA cement. Biodentine and
273 AV-modified Matreva MTA cement surfaces produced more precipitates, favored by
274 the greater calcium ions release and higher pH of the surrounding media. This is
275 consistent with another study's findings which revealed that alkaline salts greatly
276 shortened the setting time, and increased ion release, and pH values of MTA and
277 CEM cement [36].

278 Calcium phosphate deposition after immersion in HBSS indicates the amorphous or
279 crystalline precursors of carbonated apatite or hydroxyapatite. The maturation of these
280 precursors depends on the pH of the media and the time of immersion. The XRD
281 analysis of the different groups after 28 days of immersion in HBSS revealed calcium
282 hydroxide and calcium carbonate peaks. Peaks of crystalline hydroxyapatite were not
283 detected, probably due to the low percent of the crystalline apatite formed. However,
284 the results of FTIR spectra for the different groups after immersion in HBSS showed
285 characteristic bands of phosphate groups due to the deposition of the apatite
286 precursors on the material's surface. Similar findings were reported in earlier studies
287 [37,38]. Moreover, Matreva MTA's *in vivo* bioactivity could be considerably
288 enhanced by AV, generating moderate inflammation and good dentine bridge
289 development comparable to Biodentine [12].

290 **Conclusion**

291 Addition of 20 and 30% AV solutions to Matreva MTA reduced the setting time and
292 improved the handling characteristics as well as the *in-vitro* bioactivity, resembling
293 the qualities of Biodentine. Both AV-modified Matreva MTA and Biodentine cements
294 had extended alkalinizing activity and calcium ion release.

295 **Clinical relevance**

296 AV-modified Matreva MTA can be considered a promising biomaterial for different
297 endodontic applications.

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301 **Conflict of interests:**

302 The authors declare no competing interests.

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445 **Table 1:** The materials utilized in the current study

Materials	Brand name	Manufacturer	Composition	Lot number
Tricalcium silicate-based cement	Biodentine	Septodont, Saint-Maur-des-Fossés, France.	Powder: Tri-calcium silicate, di-calcium silicate, calcium carbonate and oxide (fillers), iron oxide, and zirconium oxide (radiopacifier). Liquid: Calcium chloride (accelerator), hydrosoluble polymer	B25376
	Matreva MTA	Matreva Dental Labs, Egypt.	Powder: Tri-calcium silicate, di-calcium silicate, tricalcium aluminate, Sulphur trioxide, titanium oxide, and bismuth oxide (radiopacifier). Liquid: Distilled water	11002
Aloe vera extract	Aloe Fuzion	Global Health Center, LP. Houston, Texas, USA.	Organic inner leaf Aloe	150CC

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450 **Table 2:** The mean \pm SD of flow and setting time for the various tested groups.

Parameters	Group (I) Biodentine	Group (II) Matreva MTA	Group (III) Matreva MTA 10% AV	Group (IV) Matreva MTA 20% AV	Group (V) Matreva MTA 30% AV	P-value
Flow test (mm)	11.85 \pm 0.19 ^C	12.98 \pm 0.22 ^A	12.55 \pm 0.35 ^B	11.82 \pm 0.10 ^C	11.56 \pm 0.15 ^C	<0.001*
Initial setting (min)	16.75 \pm 0.76 ^D	43.67 \pm 2.34 ^A	39.21 \pm 0.93 ^B	20.88 \pm 0.77 ^C	17.83 \pm 1.17 ^D	<0.001*
Final setting (min)	28.92 \pm 1.02 ^E	109.33 \pm 1. 75 ^A	98.67 \pm 3.01 ^B	84.33 \pm 3.39 ^C	58.83 \pm 2.64 ^D	<0.001*

451 Means with different superscript letters within the same row are statistically
452 significantly different *: significant at $P \leq 0.05$.

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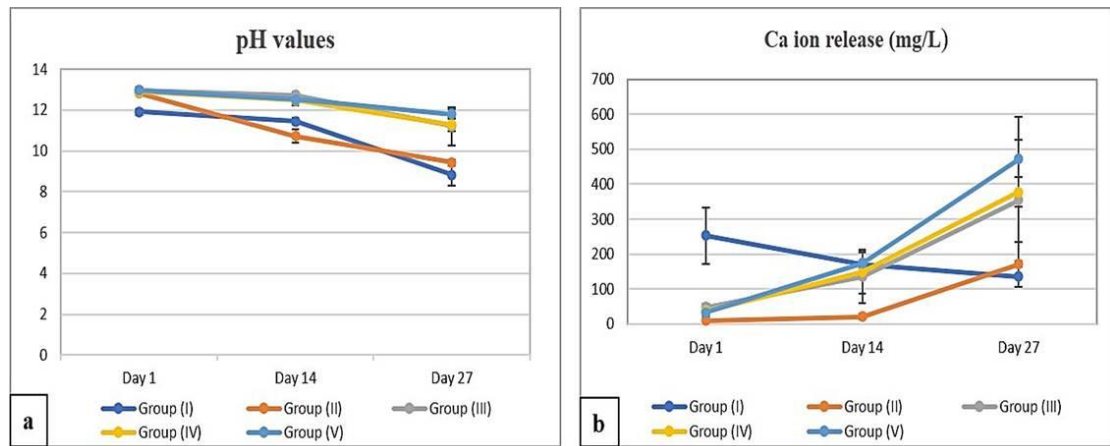
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466 **Fig. 1:** Line chart showing (a) average pH values and (b) calcium ion release values
 467 (mg/L).

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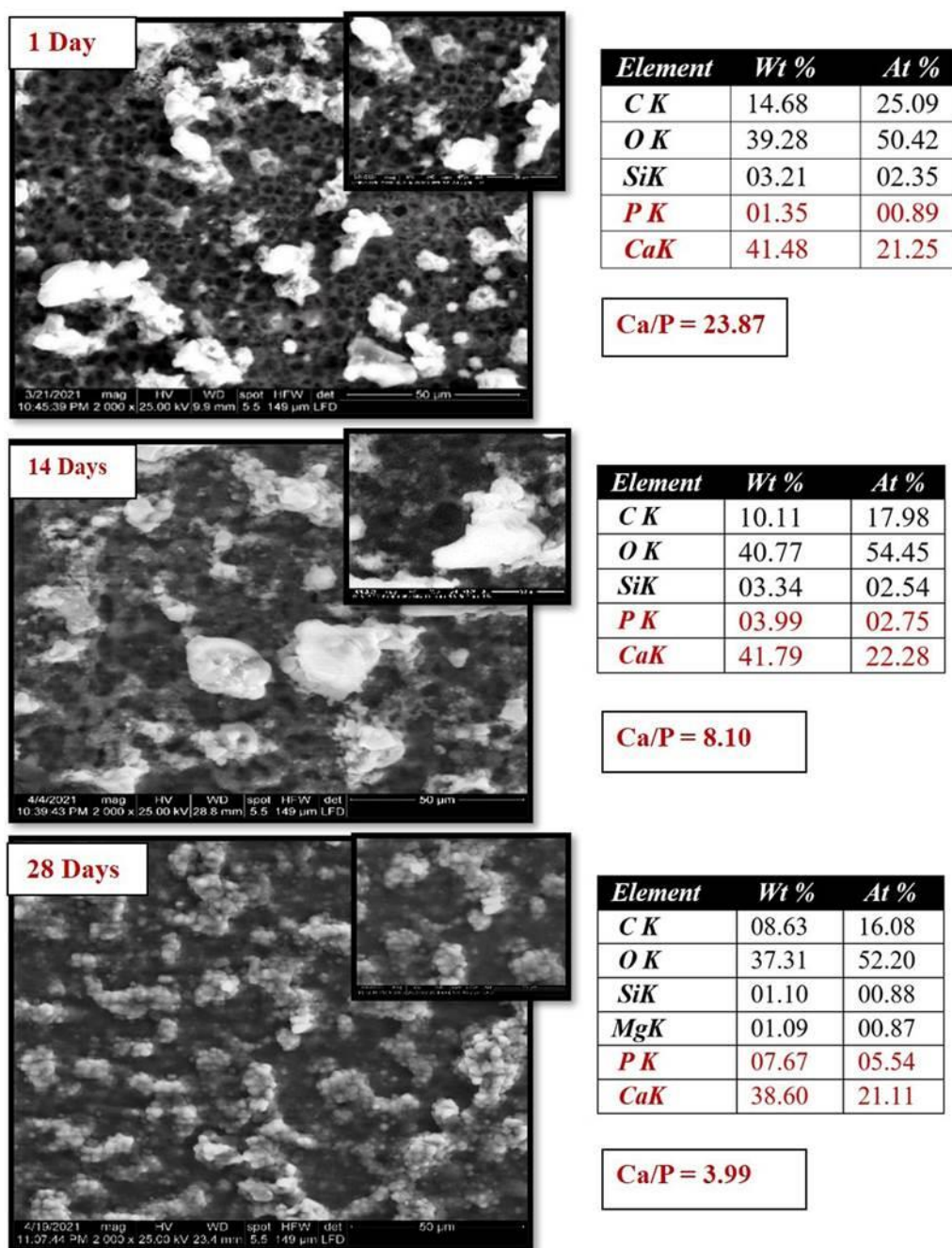
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486 **Fig. 2:** ESEM photomicrographs at different magnifications showing the surface

487 deposits over the Biodentine disc stored in HBSS for different time intervals with the

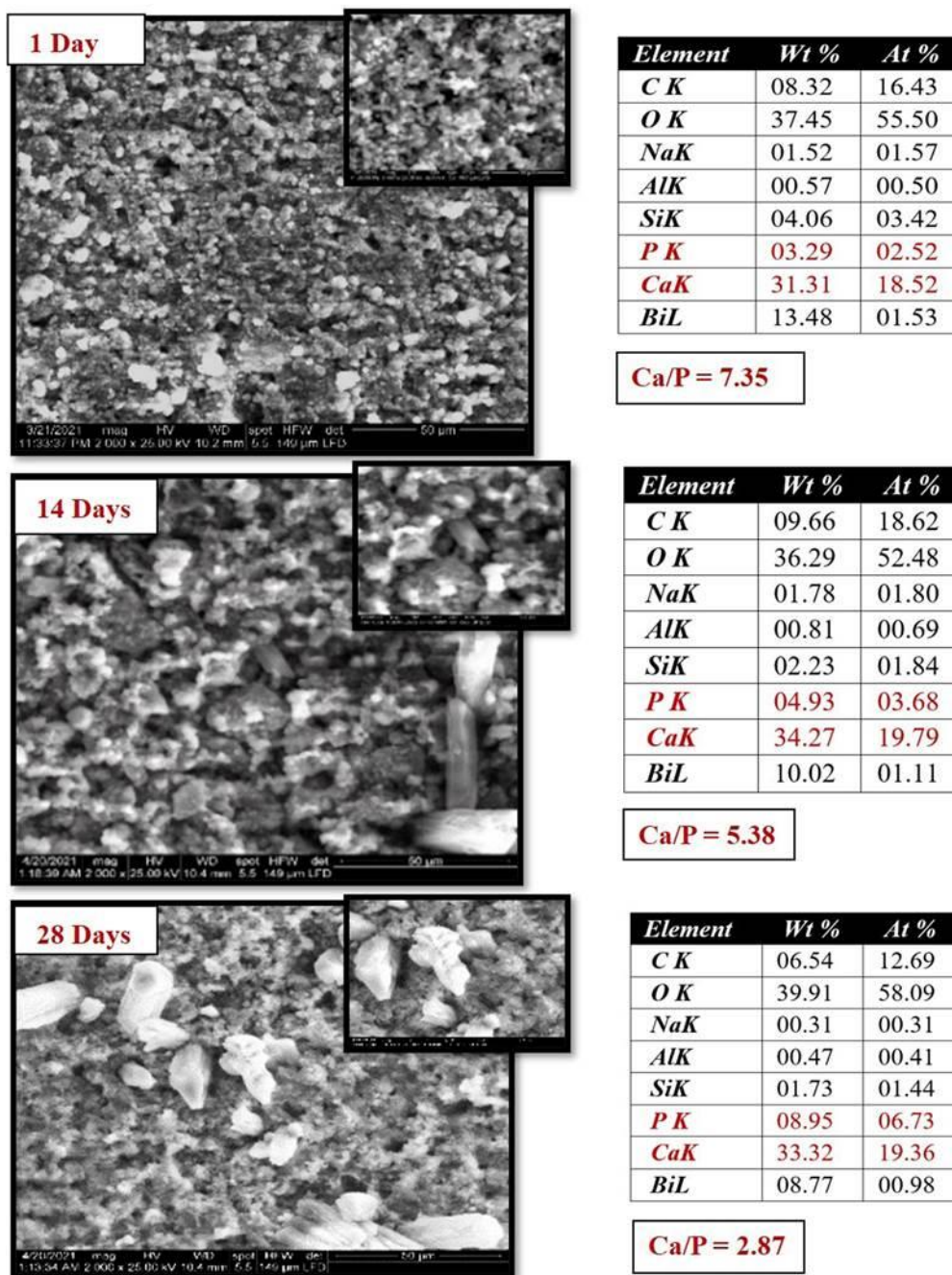
488 corresponding EDX analysis.

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494 **Fig. 3:** ESEM photomicrographs at different magnifications showing the surface

495 deposits over Matreva MTA disc stored in HBSS for different time intervals with the

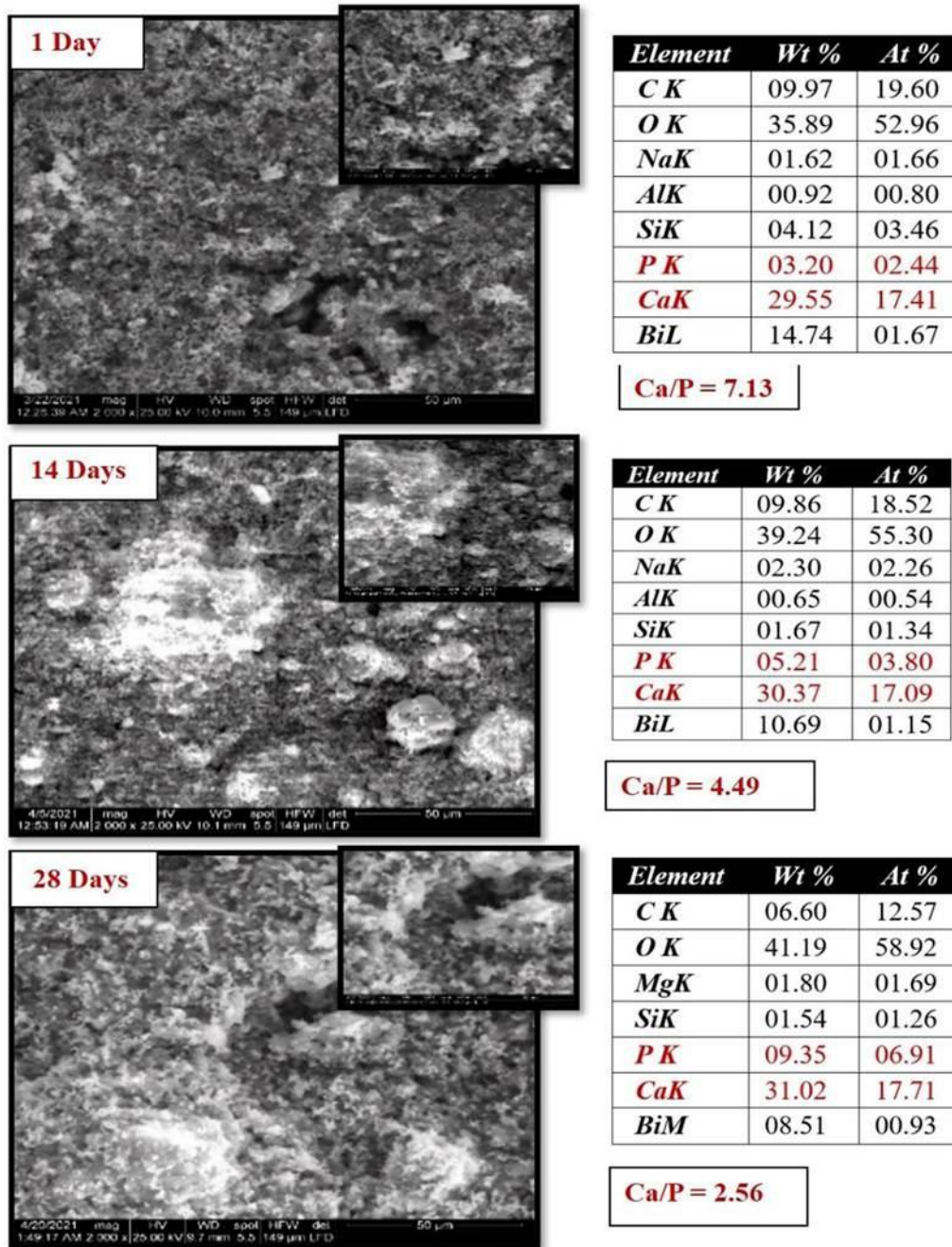
496 corresponding EDX analysis.

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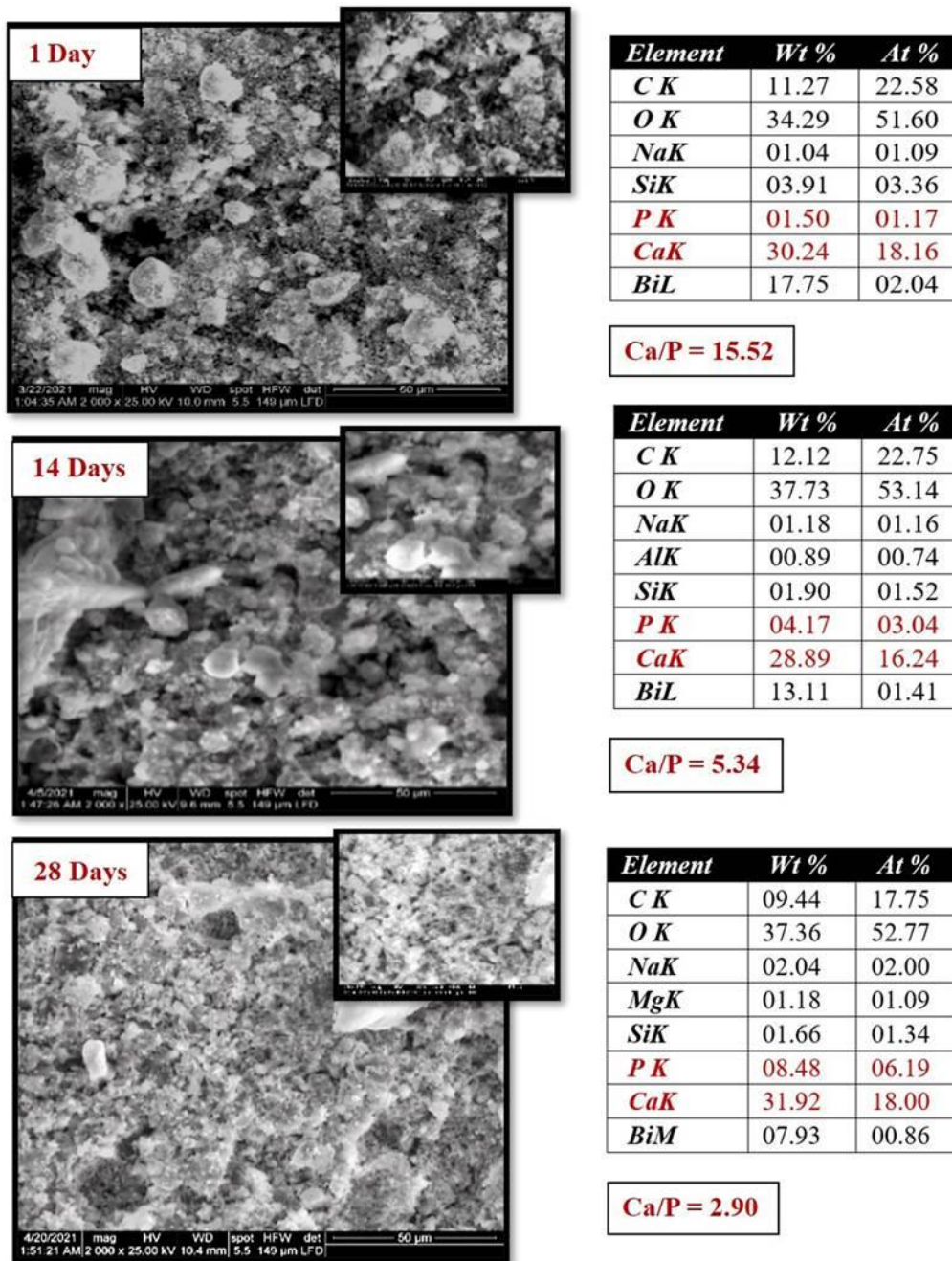
502 **Fig. 4:** ESEM photomicrographs at different magnifications showing the surface
 503 deposits over Matreva MTA with 10% Aloe Vera disc stored in HBSS for different
 504 time intervals with the corresponding EDX analysis.

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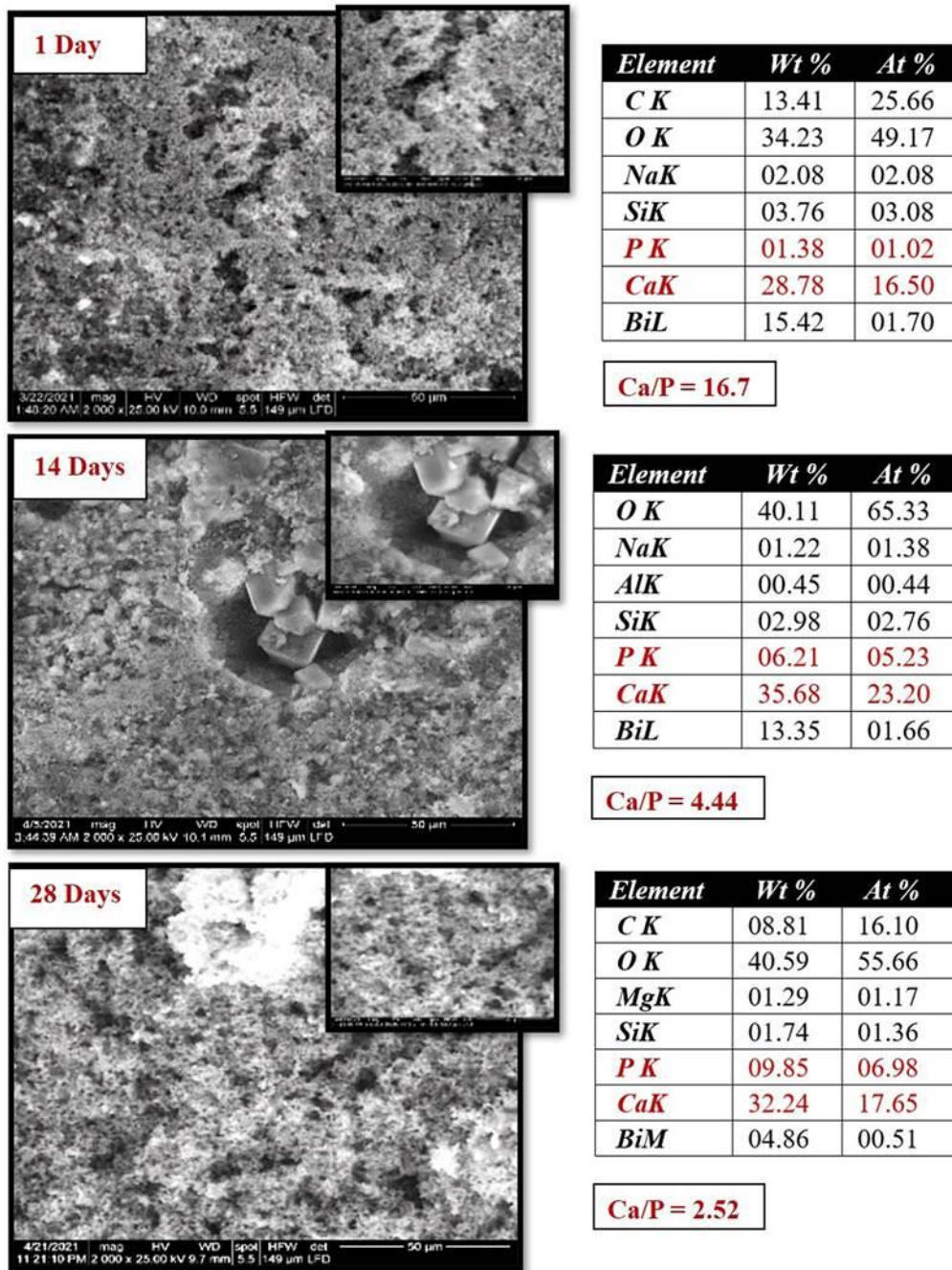
510 **Fig. 5:** ESEM photomicrographs at different magnifications showing the surface
 511 deposits over Matreva MTA with 20% Aloe Vera disc stored in HBSS for different
 512 time intervals with the corresponding EDX analysis.

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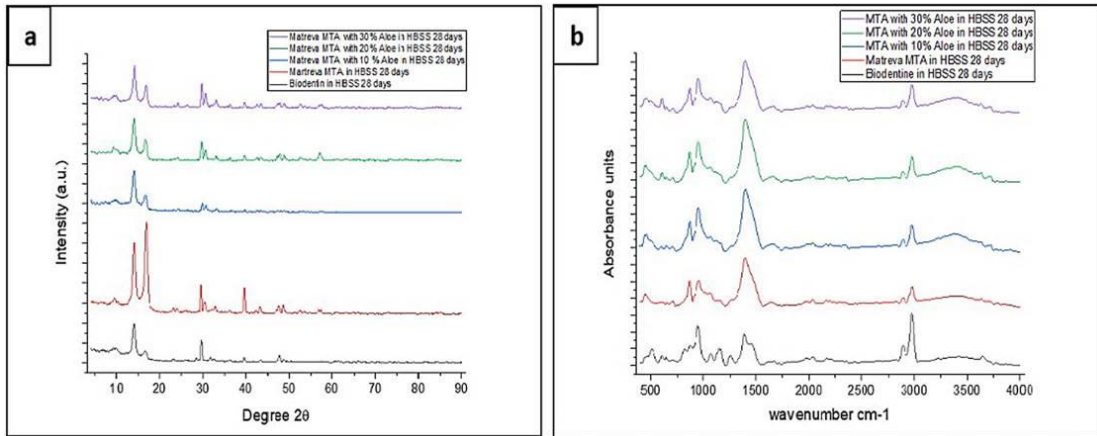
518 **Fig. 6:** ESEM photomicrographs at different magnifications showing the surface

519 deposits over Matreva MTA with 30% Aloe Vera disc stored in HBSS for different

520 time intervals with the corresponding EDX analysis.

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524 **Figure 7:** Images showing (a) XRD and (b) FTIR analysis of different groups after
 525 immersion in HBSS 28 days.

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