REVIEW

Foster®: A High-Efficiency Combination Metered Dose Inhaler with Consistent Particle Size Distribution at Alternative Flow Rates

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ABSTRACT

Introduction: This publication adds perspective to a recent publication by Johal et al. that presented the performance of combination inhalation therapies at a flow rate differing from that recommended by the regulatory authorities for metered dose inhaler (MDI) performance testing. Altering the flow rate through an impactor can create potential pitfalls which can result in performance misrepresentation.

Performance Testing of MDIs at Non-Standard Flow Rates: In-house data for Foster® (Chiesi, Parma, Italy) and Flutiform® (Bard Pharmaceuticals Limited, Cambridge, UK) have been collected using standard pharmacopaeial conditions and also at the unconventional 60 L/min flow rate utilized by Johal et al.

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D. A. Lewis (⊠) · R. Johnson · H. O'Shea Chiesi Ltd, Chippenham, Wiltshire, UK e-mail: D.Lewis@chiesi.com inhaled corticosteroids (ICS) and long-acting beta agonists in Foster MDI from approximately 1.2–0.5 μm with increase in flow rate (Johal et al.) is not observed. Use of the Andersen cascade impactor at flow rates above 28.3 L/min is not common practice. The industry generally utilizes data from the next generation impactor (NGI), an impactor specifically designed and developed for this purpose. Data for the ICS component of Foster have been generated using an NGI operated at 30 and 60 L/min, yielding an MMAD ($\pm SD$) of 1.1 \pm 0.1 μm at both flow rates.

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Therapeutic Significance of Submicron Particles: Johal et al. suggest that submicron particles are prone to be exhaled by the patient, and therefore imply that they may be non-effective. However, therapeutic significance of submicron particles is supported by a scintigraphic lung deposition study carried out using the Foster MDI. The in vivo data highlight that just 2–3% of the nominal dose was exhaled, with 31–34% deposited in the lungs.

Conclusion: Consistent particle size distribution of both active drug components

delivered from Foster MDI at flow rates of 28–30 and 60 L/min is observed.

Keywords: Metered dose inhaler; Particle size distribution; Andersen cascade impactor; Next generation impactor; Sampling flow rate; Foster; Flutiform

INTRODUCTION

Characterization of the performance of metered dose inhalers (MDIs) by cascade impaction is a complex procedure, requiring the pertinent selection of many experimental and environmental variables in order to achieve realistic and relevant results. Examples have been published illustrating that MDI delivery performance variability may occur under extreme ambient conditions [1–3].

No less crucial is appropriate analysis of the resulting data in order to calculate accurate values for performance indicators such as mass median aerodynamic diameter (MMAD) and fine particle dose (FPD) [4]. Industry approved software is available to facilitate the appropriate processing of experimental data in accordance with regulatory guidelines (CITDAS V3.10, Copley Scientific, Nottingham, UK).

This publication adds perspective to a recent publication by Johal et al. [5] that presented combination inhalation performance of therapies at a flow rate, 60 L/min., differing from that recommended by regulatory authorities for Metered Dose Inhaler performance testing, 28.3 L/min [United States Pharmacopeia (USP) 36]. Altering the flow rate through an impactor can create potential pitfalls, including impactor choice and preparation (i.e., plate coating) and data processing parameters, which can result in performance misrepresentation [2–4, 6–9].

This review article does not contain any studies with human or animal subjects performed by any of the authors.

PERFORMANCE TESTING OF MDIS AT NON-STANDARD FLOW RATES

Johal et al. [5] utilized a dosing procedure that, seemingly, is non-compliant with the patient instruction leaflet [10]. Furthermore, it is known that a combination of low dose number and uncoated impactor plates results in the underestimation of particle size information [2, 3, 6, 7]. In addition, figure two of the Johal et al. [5] paper utilizes identical impactor stage cut-off diameters for the Andersen Cascade Impactor (ACI), at both 28.3 and 60 L/min sampling flow rates, rather than calculating precise stage cut-off diameters and appropriately representing the data [8, 9]. Table 1 presents our in-house data for Foster® (Beclometasone dipropionate and Formoterol Fumarate, Chiesi, Parma, Italy) and Flutiform® (Fluticasone propionate and Formoterol Fumarate, Bard Pharmaceuticals Limited, Cambridge, UK) collected using standard pharmacopaeial conditions and also at the unconventional 60 L/min flow rate utilized by Johal et al. [5]. The data in Table 1 have been processed with ACI stage cut-off diameters in accordance with Van Oort et al. [9]. A marked reduction in MMADs of both the inhaled corticosteroids (ICS) and long-acting beta agonists (LABA) in Foster MDI from approximately 1.2-0.5 µm with increase in flow rate (Johal et al. [5]), which permits a potential misrepresentation of the product's characteristics, is not observed. Furthermore, careful inspection of the cumulative fractional frequency-LABA particle size distribution curves presented in figure 2d of their paper [5],

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Table 1 MMAD values $(n \ge 6)$ for Foster and Flutiform delivered to ACI at alternative flow rates

Product	MMAD (μm) ± standard deviation	
	28.3 L/min	60.0 L/min
Foster		
BDP	1.3 ± 0.1	1.2 ± 0.2
FF	1.4 ± 0.2	1.2 ± 0.2
Flutiform		
FP	4.0 ± 0.1	3.6 ± 0.1
FF	3.6 ± 0.1	3.2 ± 0.2

ACI Andersen cascade impactor, BDP beclometasone dipropionate, FF formoterol fumarate, FP fluticasone propionate, MMAD mass median aerodynamic diameter

would suggest that MMADs derived from these plots are consistent with those shown in Table 1. The Geometric Standard Deviation observed for the 60 L/min Foster in-house data was 1.8, well below the surprising high value of 5.3 reported by Johal et al. [5].

Use of the ACI at flow rates above 28.3 L/min is not common practice [8, 9]. The industry generally utilizes data from the next generation impactor (NGI; USP 36, Apparatus 6), an impactor specifically designed and developed for this purpose [11]. In-house data for the ICS component of Foster have been generated using an NGI operated at 30 and 60 L/min yielding an MMAD (\pm SD) of 1.1 \pm 0.1 μ m at both flow rates. The equivalence of the particle size distributions for the ICS and LABA components emitted from Foster has previously been published [12].

Johal et al. [5] report all fine particle drug delivery data normalized to nominal label claim rather than using the accepted pharmacopoeial approach of calculation against drug mass (dose), delivered to the ACI, ex-actuator, nor is it confirmed that drug mass balance against experimental delivered dose uniformity was achieved (USP 36), which is unhelpful. Furthermore, reporting that Flutiform has a

higher and more consistent fine particle fraction (FPF) than Foster is potentially misleading, firstly, because the ICS components are chemically and physically different and formulated at different concentrations, and secondly, our in-house data generated by NGI at 30 L/min show the converse as follows: Flutiform (FP as particulate suspension)—FPD = $39 \pm 4 \,\mu g$, FPF (as fraction of delivered dose) $37 \pm 4\%$; Foster (BDP as solution)—FPD = $34 \pm 2 \,\mu g$, FPF $40 \pm 2\%$. The corresponding NGI data obtained at 60 L/min are Flutiform: FPD = $39 \pm 3 \,\mu g$, FPF = $34 \pm 1\%$; Foster; FPD = $47 \pm 2 \,\mu g$, FPF = $54 \pm 2\%$.

THERAPEUTIC SIGNIFICANCE OF SUBMICRON PARTICLES

Johal et al. [5] suggest that submicron particles are prone to be exhaled by the patient, and therefore imply that they may be non-effective. However, studies exist which contradict such a claim [13–16]. Extra-fine particles have been demonstrated to show high central and peripheral deposition within the lung, as particle diffusion processes become more dominant when particle size decreases [15]. Therapeutic significance of submicron particles is supported by a scintigraphic lung deposition study carried out using the Foster MDI [13]. The in vivo data highlight that just 2–3% of the nominal dose was exhaled, with 31–34% deposited in the lungs.

The testing of MDIs at alternative flow rates is not a common practice in the pharmaceutical industry: the majority of patient instruction leaflets, including those for Foster [10] and Flutiform [17], advocate a long, slow breath when a dose is administered; for example: "breathe in slowly and deeply"; "hold your breath for as long as possible". The patient is also directed not to perform the process "too quickly".

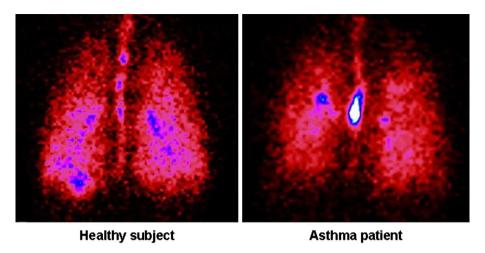


Fig. 1 Scintigraphic image of healthy subject and asthma patient after a single inhalation of four puffs of Foster (BDP/FF; 100/6), metered dose inhaler. *BDP* beclometasone dipropionate, *FF* formoterol fumarate

Figure 1 demonstrates that for subjects with alternative breath capabilities, similar drug deposition is obtained, highlighting the robustness of Foster MDI drug in vivo delivery performance for both healthy and injured lungs. Analysis of 8 patients with asthma and 8 healthy subjects showed a lung deposition of 30.9 ± 8.9 and $34.1 \pm 9.3\%$ of the nominal dose, respectively [13]. This in vivo lung deposition correlates well with published in vitro data of $35 \pm 1\%$ of nominal dose [12].

CONCLUSION

Consistent particle size distribution of both active drug components delivered from Foster MDI at flow rates of 28–30 and 60 L/min is observed.

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Conflict of interest. R. De Maria is an employee of Chiesi Farmaceutici SpA, Parma, Italy. I. Zagnoni is an employee of Chiesi Farmaceutici SpA, Parma, Italy. A. Bodria is an employee of Chiesi Farmaceutici SpA, Parma, Italy. S. Bonelli is an employee of Chiesi Farmaceutici SpA, Parma, Italy. M. Dagli Alberi is an employee of Chiesi Farmaceutici SpA, Parma, Italy. D.A. Lewis is an employee of Chiesi Ltd, Chippenham, Wiltshire, UK. R. Johnson is an employee of Chiesi Ltd, Chippenham, Wiltshire, UK. H. O'Shea is an emplovee of Chiesi Ltd. Chippenham, Wiltshire, UK.

Compliance with ethics guidelines. This review article does not contain any studies with human or animal subjects performed by any of the authors.

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