

1 **Fabrication and Characterization of Complex Coacervates Utilizing Gelatin and**
2 **Carboxymethyl Starch**

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14 **Abstract**

15 **Background:** In comparison to native polysaccharides, modified polysaccharides have greatly
16 expanded applications due to their improved compatibility and interactions with proteins and active
17 compounds in the realm of food-related areas. Nonetheless, there is a noticeable dearth of research
18 concerning the utilization of carboxymethyl starch (CMS) as a microcapsule wall material in food
19 processing despite its common use in pharmaceutical delivery. Therefore, the development of an
20 economical and safe embedding carrier using CMS and gelatin (GE) holds immense importance within
21 the food processing industry. In this work, the potential of innovative coacervates formed by the
22 combination of GE and CMS as a reliable, stable, and biodegradable embedding carrier was evaluated
23 by turbidity measurements, thermogravimetric analysis (TGA), X-ray diffraction (XRD), Fourier-
24 transform infrared (FT-IR) spectroscopy, and rheological measurements. **Results:** The results indicate
25 that GE-CMS coacervates primarily resulted from electrostatic interactions and hydrogen bonding.
26 The optimal coacervation was observed at pH 4.6 and a GE/CMS blend ratio of 3:1 (w/w). However,
27 the addition of NaCl reduced coacervation and made it less sensitive to temperature changes (35–55°C).
28 Compared to individual GE or CMS, the coacervates exhibited higher thermal stability, as shown by
29 TGA. Importantly, XRD analysis shows that the GE-CMS coacervates maintained an amorphous
30 structure. Rheological testing reveals that the GE-CMS coacervates exhibited shear-thinning behavior
31 and gel-like properties. **Conclusion:** Overall, attaining electroneutrality in the mixture boosts the
32 formation of a denser structure and enhances rheological properties, leading to promising applications
33 in food, biomaterials, cosmetics, and pharmaceutical products.

34 **Keywords:** Gelatin carboxymethyl starch coacervates; Natural Polymers; Microcapsule wall material;
35 Polyelectrolyte complexation; Food processing; Active compounds delivery

36 **1. Introduction**

37 Proteins and polysaccharides, natural compounds extensively used in the food industry ¹, have a
38 natural tendency to interact due to their amphiphilic characteristics. When these two biopolymers come
39 into contact, they can exhibit varying degrees of interaction. Typically, thermodynamic compatibility
40 (attraction) and/or incompatibility (repulsion) emerge between biopolymers and solvents ².
41 Thermodynamic incompatible interactions mainly occur at high ionic strength and concentration levels,
42 and therefore, extensive attention has been directed towards achieving thermodynamic compatibility,
43 characterized by low ionic strength and low concentration, resulting in the formation of soluble
44 complexes or condensates ³.

45 Studies have shown that protein-polysaccharide complexes are formed under different conditions,
46 including pH, ionic strength, temperature, the concentration of biopolymers, and the molecular
47 characteristics of these biopolymers, like charge density and molecular weight (M_w) ^{4,5}. Moreover, the
48 polymers formed by protein and polysaccharides offer many advantages, such as high load and stability.
49 The complexes can serve as effective delivery systems to protect bioactive compounds, such as
50 essential oils ⁶, vitamins ⁷, and probiotics ⁸.

51 Starch is widely recognized as a highly promising material for the development of novel carriers,
52 owing to its advantages like binding properties, cost-effectiveness, and widespread availability ⁹.
53 Despite its remarkable features, starches still have some shortcomings, such as limited solubility in
54 cold water, which restricts its application in food delivery. In recent years, researchers have expanded
55 the range of wall materials by using modified polysaccharides to enhance compatibility and promote
56 interactions with proteins and active compounds, in addition to employing native polysaccharides ¹⁰.
57 Chemical modification of starch offers an excellent avenue to create new starch derivatives with

58 enhanced properties. Carboxymethyl starch (CMS), a frequently investigated modified starch, is a
59 negatively charged polysaccharide with a wide range of promising applications owing to its pH
60 stability, cold water solubility, renewability, and biodegradability ¹¹. CMS, a negatively charged ether
61 derivative, can effectively retain hydrophilic or hydrophobic core materials within the carrier cavity
62 through electrostatic interactions and hydrogen bonding. Previous investigations have demonstrated
63 its potential in the oral delivery of bioactive compounds through techniques like chemical crosslinking
64 ¹². CMS has been used to fabricate innovative delivery systems covalently crosslinked with chitosan
65 hydrochloride ¹³ and polyelectrolyte complex (PEC) microparticles with chitosan for targeted drug
66 delivery ¹⁴.

67 Gelatin (GE) is a protein obtained through the partial hydrolysis of collagen. It can be
68 enzymatically degraded into various amino acids, resulting in the absence of harmful by-products.
69 Gelatin holds a "generally recognized safe" (GRAS) status conferred by the US Food and Drug
70 Administration (FDA) thanks to its non-toxic, non-carcinogenic, biodegradable, and environmentally
71 friendly nature ¹⁵. Notably, gelatin is an amphoteric protein whose molecules contain 13% positively
72 charged amino acids (arginine and lysine) and 12% negatively charged amino acids (aspartate and
73 glutamate) ¹⁶. This gives gelatin a net positive charge when the pH is below its isoelectric point (pI).
74 Gelatin-based electrostatic complexes remain the preferred choice for carriers in commercial
75 applications, attributed to their excellent emulsifying capabilities, high stabilizing activity, water
76 solubility, and significant crosslinking potential through their primary amino groups.

77 Numerous studies have explored the coacervation of gelatin with various biomacromolecules,
78 including sodium carboxymethyl cellulose (CMC) ¹⁷, sodium alginate ¹⁸, and Persian gum ¹⁹. However,
79 while there has been extensive research on carboxymethyl starch as a pharmaceutical delivery carrier

80 material recently ²⁰⁻²², there is a limited body of work on its application as a wall material for
81 microcapsules in food processing. Therefore, this study established a complex coacervation system of
82 CMS and GE to investigate the interaction mechanism between them as new wall materials. This offers
83 valuable theoretical insights for the application of the new wall material system in the encapsulation
84 of active compounds, particularly in the food and related industries. The influence of pH, temperature,
85 total biopolymer concentration, ionic strength, and GE/CMS blend ratio ($R_{GE/CMS}$) on the interaction
86 of GE-CMS mixtures was investigated through turbidity analysis. Besides, various analytical
87 techniques were employed to characterize the physicochemical properties of GE-CMS complexes,
88 including Fourier transform infrared (FT-IR) spectroscopy, X-ray diffractometry (XRD), and
89 thermogravimetric analysis (TGA). Furthermore, the rheological properties of GE-CMS complexes
90 were also measured. It is believed that this study will provide helpful information to enhance the
91 application of starch-based delivery systems through electrostatic interactions.

92 **2. Materials and methods**

93 **2.1. Materials**

94 Maize starch, containing 12.8% moisture and 27.5% amylose, was sourced from National Starch
95 Pty Ltd. Gelatin (GE, type B, Bloom 200) was supplied by Boyang Biotechnology Co., Ltd. Sodium
96 chloroacetate was purchased from Shanghai McLin Biochemical Technology Co., Ltd. All other
97 chemicals used were of analytical grade.

98 **2.2. Preparation of carboxymethyl starch (CMS)**

99 To prepare CMS, firstly, 8 g regular maize starch (RMS) and 60 mL of 80% (v/v) ethanol were
100 added in a three-necked flask under continuous stirring, followed by a slow addition of 3.61 g sodium
101 hydroxide. The reaction was maintained at 30 °C for 60 min. Then, 12.6 g of sodium chloroacetate

102 was introduced, and the mixture was stirred at 40 °C for 3 h. After completing the reaction, any
103 unreacted sodium hydroxide was neutralized using glacial acetic acid. The resulting mixture was
104 filtered, and the slurry was washed with an 80% ethanol aqueous solution until no chloride ions were
105 detected (confirmed with 0.2 M AgNO₃). The resulting precipitate was dried in an oven at 40 °C for
106 24 h and subsequently ground into a fine powder, passing through a 100-mesh sieve. The degree of
107 substitution (DS) of the prepared CMS was 0.76.

108 **2.3. Preparation of biopolymer solution**

109 A certain quantity of gelatin was dissolved in deionized water and allowed to soak for 2 h to
110 achieve full swell. Then, it was heated at 60 °C for 30 min. The CMS solution was stirred using
111 magnetic force at room temperature for 4 h and then refrigerated overnight at 4 °C to ensure complete
112 hydration.

113 **2.4. ζ -Potential measurement**

114 A zetasizer (Nano-ZS, Malvern Instruments Ltd, Malvern, Worcestershire, UK) was used to
115 measure the ζ -potentials of samples at a concentration of 0.1% (w/v) under different pH conditions.

116 **2.5. Turbidity measurement**

117 Turbidity measurements were utilized to study the GE-CMS interaction behavior. The pH of the
118 solutions was adjusted using acetic acid (10%, v/v) through an injector. The mass mixing ratio ($R_{GE/CMS}$)
119 was varied from 1:1 to 5:1 at a total concentration of 0.1% (w/v). The total concentration in this study
120 ranged from 0.05% to 0.1% at a constant $R_{GE/CMS}$ of 3:1. Temperature was varied in the range of 35–
121 50 °C, and ionic strength was adjusted from 0 to 10 mM. Turbidity analysis was performed using a
122 UV-vis spectrophotometer (UV-3802, Unico Instruments Corporation, Shanghai, China) at 600 nm.
123 Deionized water was used as a blank for all tests.

124 **2.6. FT-IR spectroscopy**

125 The FT-IR spectra of RMS, GE, CMS, and GE-CMS complex coacervates were acquired using
126 FT-IR spectroscopy (VERTEX 70, BRUKER, Germany). Each sample was mixed with KBr powder.
127 The frequency range was set from 4000 to 400 cm^{-1} with a resolution of 4 cm^{-1} .

128 **2.7. X-ray diffraction (XRD)**

129 The powder was characterized using a Rigaku Ultima IV X-ray diffractometer operating at 40 kV
130 and 40 mA. Diffractograms were collected in reflection mode within a range of 4° to 50° at a scanning
131 speed of 2 °/min.

132 **2.8. Thermogravimetric analysis (TGA)**

133 The thermal stability of GE, CMS, and GE-CMS coacervates was determined using a TGA
134 instrument (TG 209 F1 Libra, German). The parameters for the analysis were as follows: The
135 temperature range was set from 35 °C to 500 °C with a heating rate of 20 °C/min, and a nitrogen flow
136 rate of 20 mL/min was maintained.

137 **2.9. Rheological measurement**

138 Dynamic rheological properties of GE-CMS complexes were assessed using a HAAKE MARS
139 60 rheometer (Thermo Fisher Scientific, USA). The GE-CMS coacervates were loaded onto the plate
140 and allowed to equilibrate for 3 min. Strain sweep tests were first carried out to determine the linear
141 viscoelastic region of the samples, and a constant strain value of 1% was selected for the subsequent
142 frequency sweep tests. Dynamic viscoelastic properties of GE-CMS coacervates were measured over
143 a frequency range from 0.1 to 10 Hz. Viscosity was measured using a steady shear rate sweep, and the
144 temperature was set at 25°C.

145 **2.10. Statistical analysis**

146 The experimental data were presented as the mean \pm standard deviation (SD) based on at least
147 triplicate measurements. Statistical analysis was performed using Origin 2021 and SPSS 26.0 software.
148 Duncan's HSD test ($p < 0.05$) was used to determine significant differences.

149 **3. Results and discussions**

150 **3.1. Effect of pH on the ζ -potential of gelatin and carboxymethyl starch**

151 The pH plays a crucial role in complex coacervation, impacting the charge interactions between
152 proteins and polysaccharides²³. **Fig. 1** illustrates the pH-dependent ζ -potential of 0.1% GE and CMS.
153 CMS showed a negative zeta potential, decreasing from -15 to -39 mV as the pH increased due to
154 carboxylic group deprotonation. In contrast, GE showed a decreasing trend as pH gradually increased,
155 shifting from positive to negative at pH 5.25, which is the pI of gelatin. At $\text{pH} < \text{pI}$ (5.25), gelatin
156 becomes positively charged due to the protonation of amino groups and the neutralization of
157 carboxylate groups. These measurements show that GE and CMS carry opposite charges within the
158 pH range of 5.25 to 3, suggesting potential electrostatic complexation between these biopolymers in
159 this pH range.

160

161 **3.2. Turbidity measurement: Factors influencing the complex coacervation of gelatin and** 162 **carboxymethyl starch**

163 **3.2.1 Effects of biopolymer concentration and mass ratio**

164 Turbidity measurement provides valuable insights into the coacervation progress. **Fig. 2A** shows
165 the effect of varying the total biopolymer concentration on GE-CMS complexes under different pH
166 conditions. The total biopolymer concentrations, ranging from 0.05 to 0.1% (w/w), were measured at

167 a fixed 3:1 biopolymer mixing ratio in the absence of NaCl. The maximum turbidity values increased
168 as the total biopolymer concentration rose. Specifically, a higher concentration of total biopolymer in
169 the solution means that more positively charged protein fragments can interact with the anionic sites
170 on CMS chains.

171 Furthermore, all these curves presented a similar trend, with maximum turbidity occurring at
172 nearly 4.6 (**Fig. 2B**), indicating that pH-absorbance behavior is independent of the total biopolymer
173 concentration. These results align with previous research on casein/gum tragacanth mixtures ²⁴.
174 Previous reports have revealed that at higher total biological concentrations, an increased presence of
175 counter ions in the solution can effectively shield the charged sites on the surface of biological
176 macromolecules ^{25, 26}. Therefore, the 0.1% total biopolymer concentration was selected for further
177 investigations into the factors influencing the turbidity of GE-CMS coacervates.

178 The impact of mass ratio ($R_{GE/CMS} = 1:1-5:1$) on complex coacervation was studied at a 0.1%
179 total biopolymer concentration without the addition of sodium chloride. As shown in **Fig. 2C**, the
180 turbidity curve shifted towards a higher pH value with an increase in the mixing ratio. With $R_{GE/CMS} >$
181 4, the pH of the soluble complex formed was higher than the pI of GE (Fig. 2D). As $R_{GE/CMS}$ decreased,
182 the acidity of the solution gradually increased, indicating a greater requirement for GE's positive ions
183 to neutralize the excess negative charge ($-COO^-$) of CMS. When the mixing ratio was 3:1, the
184 maximum turbidity was attained. Hence, it can be inferred that CMS chains became saturated and
185 adsorbed by gelatin, showing the strongest electrostatic interaction.

186 The critical pH values (the pH value at which the slope of the turbidity curve first changes, pH_c ;
187 the pH value corresponding to a sudden increase in the slope of the turbidity curve, $pH_{\phi 1}$; and the pH
188 value corresponding to the maximum turbidity, pH_{opt}) shifted to higher pH values as the mixing ratio

189 increased from 1:1 to 5:1 (**Fig. 2D**), confirming that an increased mixing ratio enhanced the formation
190 of GE-CMS coacervates. Actually, polysaccharides may not require a large number of positive charges
191 to form complexes, and their stability reached a plateau with a further increase in biopolymer mixing
192 ratio ²⁷.

193 194 **3.2.2. Effects of NaCl concentration (C_{NaCl}) and temperatures**

195 **Fig. 3A** presents the turbidity curves of GE-CMS coacervates at different C_{NaCl} . The maximum
196 turbidity was observed at pH 4.6 in the absence of NaCl. However, as C_{NaCl} increased, the turbidity
197 decreased, consistent with findings on ovalbumin and propylene glycol alginate coacervates ²⁸. The
198 consistent reduction in the turbidity with increasing C_{NaCl} can be explained by a competition
199 mechanism. The addition of NaCl introduced Na^+ ions to compete with the positively charged sites of
200 GE for binding with CMS, while Cl^- ions competed with the negatively charged sites of CMS to bind
201 to GE. As a result, the binding affinity between gelatin and carboxymethyl starch gradually diminished.

202 A shift toward lower pH in critical pH was observed with increasing C_{NaCl} (**Fig. 3B**), indicating a
203 lower degree of electrostatic attraction and a greater need for acidity for complex coacervation.
204 However, pH_{ϕ_2} , the pH value corresponding to the stable slope of the turbidity curve, shifted to higher
205 pH values, and the range between pH_{ϕ_1} and pH_{ϕ_2} for biopolymer interactions reduced. Another study
206 suggested that the reduction in pH range between pH_{ϕ_1} and pH_{ϕ_2} was attributed to ion screening of the
207 protein-polysaccharide charges ²⁹.

208 The relationship between turbidity and pH was also examined at critical temperatures (35–55°C).
209 As shown in **Fig. 3C**, the turbidity of the GE-CMS complexes increased as the temperature reached
210 40 °C, possibly due to the higher solubility of gelatin. This leads to the exposure of more hydrophobic

211 groups in the aqueous solution, facilitating the participation of phenolic hydroxyl groups in the reaction.
212 However, as the temperature continued to rise, the turbidity values decreased, and critical pH values
213 shifted to lower pH values (**Fig. 3D**), potentially related to a decrease in hydrogen bonding³⁰. Liu et
214 al.³¹ also observed a correlation between critical pH values and temperature, which decreased with
215 increasing temperature. Changes in temperature had a minimal effect on the turbidity curve of the GE-
216 CMS complexes, indicating that hydrophobic interaction is not the primary driving force behind the
217 GE-CMS complexes.

218

219 **3.3. Fourier-transform infrared (FT-IR) spectroscopy analysis of the complex coacervation of** 220 **gelatin and carboxymethyl starch**

221 **Fig. 4A** displays the infrared spectra of RMS, GE, CMS, and GE-CMS coacervates. Compared
222 to RMS, the spectrum of CMS showed a new absorption peak in the range of 1300–1600 cm^{-1} . The
223 absorption peaks at 1590 cm^{-1} and 1409 cm^{-1} could be attributed to carbonyl functional groups,
224 confirming the occurrence of starch carboxymethylation. Similar results were observed in
225 carboxymethylated kudzu starch³². The infrared absorption peaks of gelatin induced a characteristic
226 band at 3407 cm^{-1} resulting from N-H and O-H vibrations³³. Additionally, the peaks at 1629 cm^{-1}
227 (C=O band vibration of amide I), 1526 cm^{-1} , and 1229 cm^{-1} represented amide II and amide III,
228 respectively³⁴. The spectrum of GE-CMS coacervate closely resembled that of gelatin, with some
229 absorption peaks shifting. Notably, the N-H bands of GE (3270 cm^{-1}) shifted to 3294 cm^{-1} , indicating
230 that the amide group of GE might have formed strong hydrogen bonds with the hydroxyl group of
231 CMS during the coacervation process. These results align with previous research³⁵.

232 Furthermore, the amide II band in gelatin exhibited a shift from 1526 cm^{-1} to 1540 cm^{-1} ,

233 corresponding to the disappearance of the -NH_3 vibration peak in gelatin. The most significant change
234 occurred in the amide I band, shifting from 1629 cm^{-1} to 1640 cm^{-1} . This change is attributed to the
235 electrostatic interaction between the carboxyl groups of CMS and the amino groups of GE, indicating
236 the occurrence of complex coacervation. This change may be related to the transformation of the
237 protein from the α -helical structure to more organized β -sheet and amorphous structures³⁶, indicating
238 the occurrence of complex coacervation. A similar slight shift has also been observed in egg proteins-
239 xanthan gum mixtures³⁷.

240 In addition, the absorption peak representing the symmetric and asymmetric stretching vibrations
241 of carboxyl groups (1590 cm^{-1} and 1409 cm^{-1}) disappeared upon the forming of GE-CMS coacervates.
242 This suggests that in the presence of proteins, carbohydrate molecules have a reduced ability to form
243 intermolecular hydrogen bonds³⁸. Therefore, it can be concluded that GE-CMS coacervates formed
244 mainly through hydrogen bonding and electrostatic interaction.

245

246 **3.4. X-ray diffraction (XRD) analysis of the complex coacervation of gelatin and carboxymethyl** 247 **starch**

248 Assessing whether a substance is in an amorphous or crystalline state is important for evaluating
249 the stability of dried products. The XRD patterns of gelatin, CMS, and their coacervates are shown in
250 **Fig. 4B**. Gelatin showed distinct broad peaks at 20.92° and 7.75° , which correspond to the triple helical
251 crystal structure of collagen³⁹.

252 Notably, both GE and GE-CMS coacervates share similar XRD patterns, highlighting the high
253 compatibility between gelatin and CMS. However, there is a reduction in the intensity of XRD peaks
254 at 20.92° and 7.75° for the GE-CMS complexes. Interactions with polysaccharides can induce

255 structural changes in proteins. Previous studies have shown that the formation of xanthan gum–gelatin
256 coacervates could change protein structures by disrupting the compact molecular arrangement of
257 gelatin chains⁴⁰. Ghobadi et al.³⁵ also observed a decrease in diffraction peak intensity when Alyssum
258 homolocarpum seed gum was added to Grass pea (*Lathyrus sativus*) protein isolates due to the
259 formation of hydrogen bonds between these two biopolymers.

260 Importantly, the GE-CMS coacervates maintain their amorphous structures. Amorphous
261 structures are known for their higher soluble and hygroscopic properties. Furthermore, they promote
262 the efficient release of core materials within capsules.

263

264 **3.5. Thermogravimetric analysis (TGA) analysis of the complex coacervation of gelatin and** 265 **carboxymethyl starch**

266 As depicted in **Fig. 5**, all samples exhibited a two-step weight loss pattern during thermal analysis.
267 The first minor mass reduction, occurring at approximately 100 °C, was primarily due to water
268 evaporation from the biopolymers. Subsequently, the second step in weight loss is associated with the
269 decomposition of these biopolymers.

270 Specifically, CMS started to undergo a substantial weight reduction in the temperature range of
271 225-314 °C due to the degradation of the backbone, involving processes such as carbonization and ash
272 formation. Previous studies have indicated that CMS showed relatively low thermal stability,
273 particularly when it had a high DS⁴¹. When heated to 500 °C, CMS retains only about 50% of its initial
274 weight.

275 In contrast, gelatin demonstrated high-temperature stability and underwent significant weight loss
276 at temperatures ranging from 267 to 374 °C, with a derivative thermogravimetric (DTG) curve peak at

277 342 °C (**Fig. 5B**), which corresponds to degradation temperature (T_d). This weight loss can be
278 attributed to the cleavage of covalent peptide bonds in the gelatin structure⁴². Gelatin residue accounts
279 for about 28% of its initial weight when heated to 500 °C, aligning with previous findings⁴³.

280 In contrast to CMS and gelatin, the GE-CMS coacervates showed a more gradual weight loss
281 profile and retained about 34% of their weight even at 500 °C. The decomposition temperature of
282 coacervates was 44 °C higher than CMS, and this enhanced thermal stability can be attributed to the
283 effective molecular interactions between CMS and GE within the coacervates. Notably, the coacervates
284 did not undergo thermal decomposition until reaching temperatures as high as 251 °C, indicating
285 significantly improved thermal stability compared to their individual components.

286

287 **3.6. Rheological properties of the complex coacervation of gelatin and carboxymethyl starch at** 288 **different conditions**

289 **3.6.1 Effect of pH**

290 The apparent viscosity of GE-CMS coacervates at different coacervation pH levels is presented
291 in **Fig. 6A**. The coacervates exhibit relatively high viscosity, exceeding 100 Pa/s at low shear rates.
292 Furthermore, they displayed shear-thinning behavior, likely attributed to the structural relaxation
293 within the polysaccharides⁴⁴. Notably, the coacervates reached their highest viscosity at pH 4.6, mainly
294 due to the enhanced interactions between GE and CMS.

295 Oscillatory measurements provided information about the viscoelastic behavior of the
296 coacervates. As can be seen from **Fig. 6B**, the elastic modulus was higher than the viscous modulus
297 ($G' > G''$), indicating a gel-like character. This gel-like network structure aligns with previous findings
298 in sodium caseinate-gum tragacanth coacervates⁴⁵. In contrast, whey protein-puka gum exhibited a

299 more viscous behavior ⁴⁶. Therefore, a rheological study of different coacervates is instrumental in
300 understanding their internal structure. Notably, the values of G' and G'' reached their maxima at pH
301 4.6, in line with previous research ⁴⁷ suggesting that coacervates collected at their pH_{max} exhibit the
302 highest gel strength as a result of the tighter structures resulting from stronger electrostatic attraction.

303 **3.6.2 Effect of C_{NaCl}**

304 The apparent viscosity of GE-CMS coacervates at different C_{NaCl} is shown in **Fig. 6C**. The shear-
305 thinning behavior remained unchanged with the addition of NaCl, but the apparent viscosity decreased
306 as C_{NaCl} increased. This phenomenon can be attributed to salt ions shielding the charges of the
307 biopolymer, leading to a more relaxed coacervate structure and reduced viscosity. Moreover, the
308 presence of sodium chloride tended to increase the water content in the coacervates, further
309 contributing to their looser structure.

310 The modulus (G' and G'') of the coacervates increased with frequency and remained roughly
311 parallel, indicating weak gel-like characteristics in the binding of gelatin to CMS. Interestingly, these
312 modulus values decreased with increasing C_{NaCl} from 0 to 10 mM, indicating that the presence of salt
313 ions shields the biopolymer charges, weakening the electrostatic interaction between protein and
314 polysaccharide. It has been observed that low concentrations of salt ions can shield the repulsive forces
315 between proteins and polysaccharides, facilitating molecular binding and enhancing the modulus of
316 the composite condensate ⁴⁸. Ovalbumin-carboxymethylcellulose coacervates, for instance, showed
317 the maximum values of G' and G'' values at a salt ion concentration of 20 mM ⁴⁹. Therefore, it can be
318 inferred that the rheological properties of a colloidal system are often closely related to its internal
319 structure.

320

321 **4. Conclusion**

322 In this study, the complex coacervates based on gelatin and CMS were prepared and thoroughly
323 characterized, including turbidity analysis, TGA, XRD, FT-IR, and rheology, to elucidate the
324 interaction mechanism between these two biopolymers. The FT-IR analysis reveals that GE-CMS
325 coacervates were primarily formed through electrostatic interactions and hydrogen bonding under
326 specific conditions. Notably, the strongest electrostatic interaction of GE-CMS coacervation was
327 observed at a $R_{GE/CMS}$ of 3:1 (w/w) and pH 4.6. Additionally, the coacervates exhibited the highest
328 viscosity at pH 4.6, mainly due to the stronger interactions between GE and CMS, which aligns with
329 the results of turbidity measurements. Compared to individual GE and CMS, the GE-CMS coacervates
330 showcased greater thermodynamic stability according to TGA. Moreover, XRD analysis reveals that
331 the GE-CMS coacervates maintained their amorphous structure. These findings hold significant
332 implications, providing valuable theoretical support for the utilization of GE and CMS interactions in
333 various applications, such as foods, biomaterials, cosmetics, and pharmaceutical products.

334

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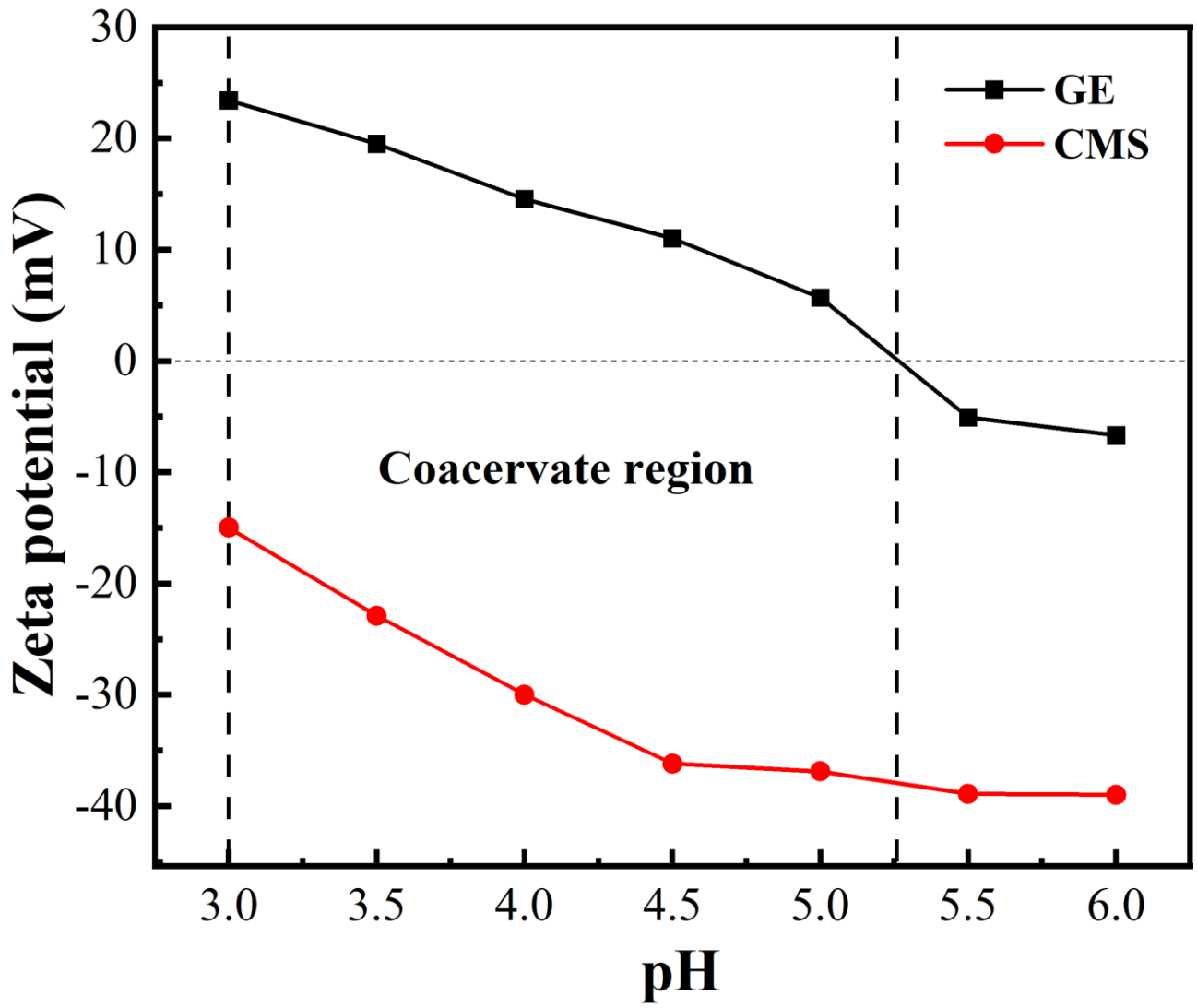


Fig. 1. ζ -potential of GE and CMS at different pH values.

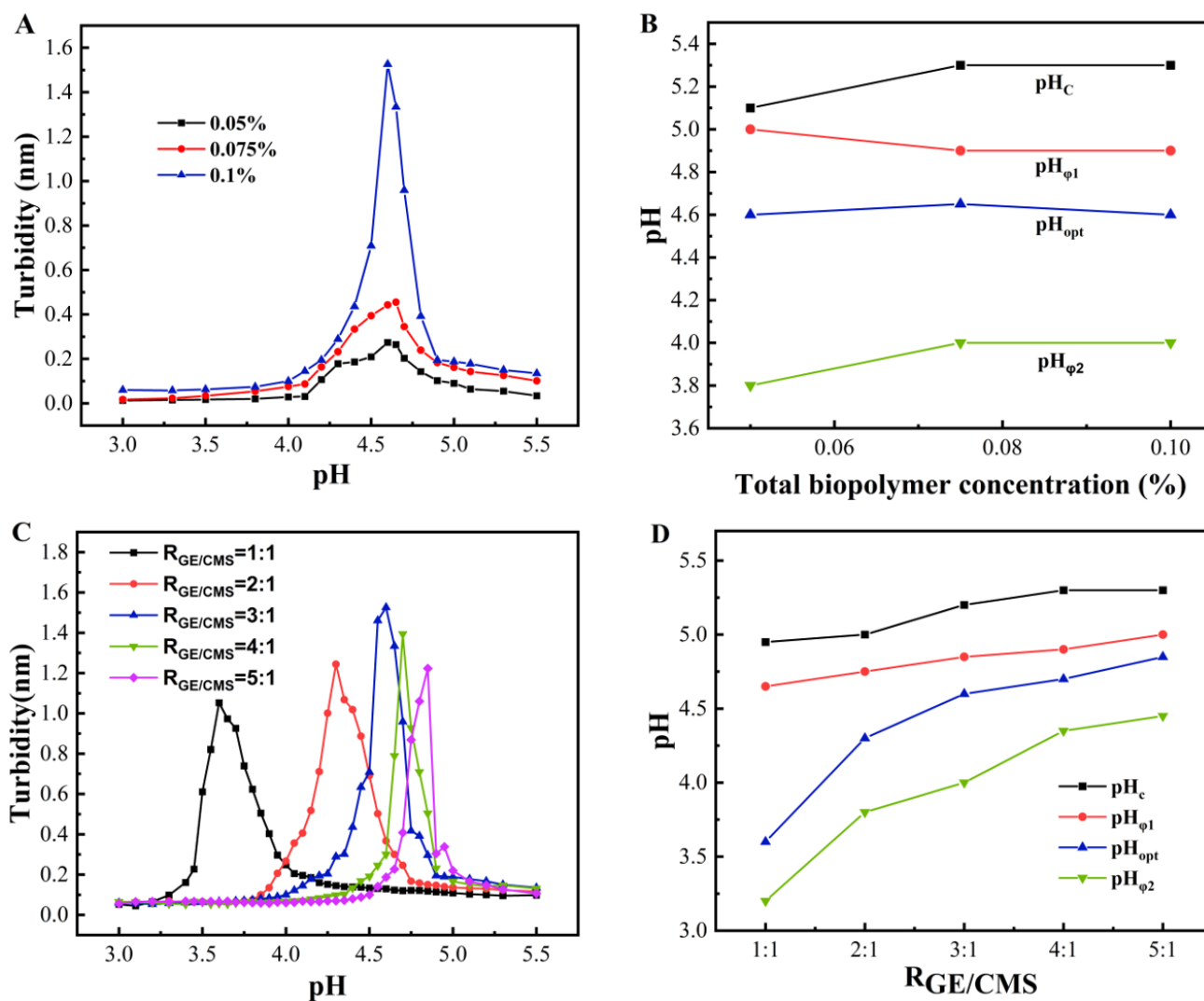


Fig. 2. Turbidity results of GE-CMS mixtures at different biopolymer concentration (A) and different mass ratios (C); critical pH values according to the biopolymer concentration (B) and the mass ratio (D) of GE-CMS mixtures.

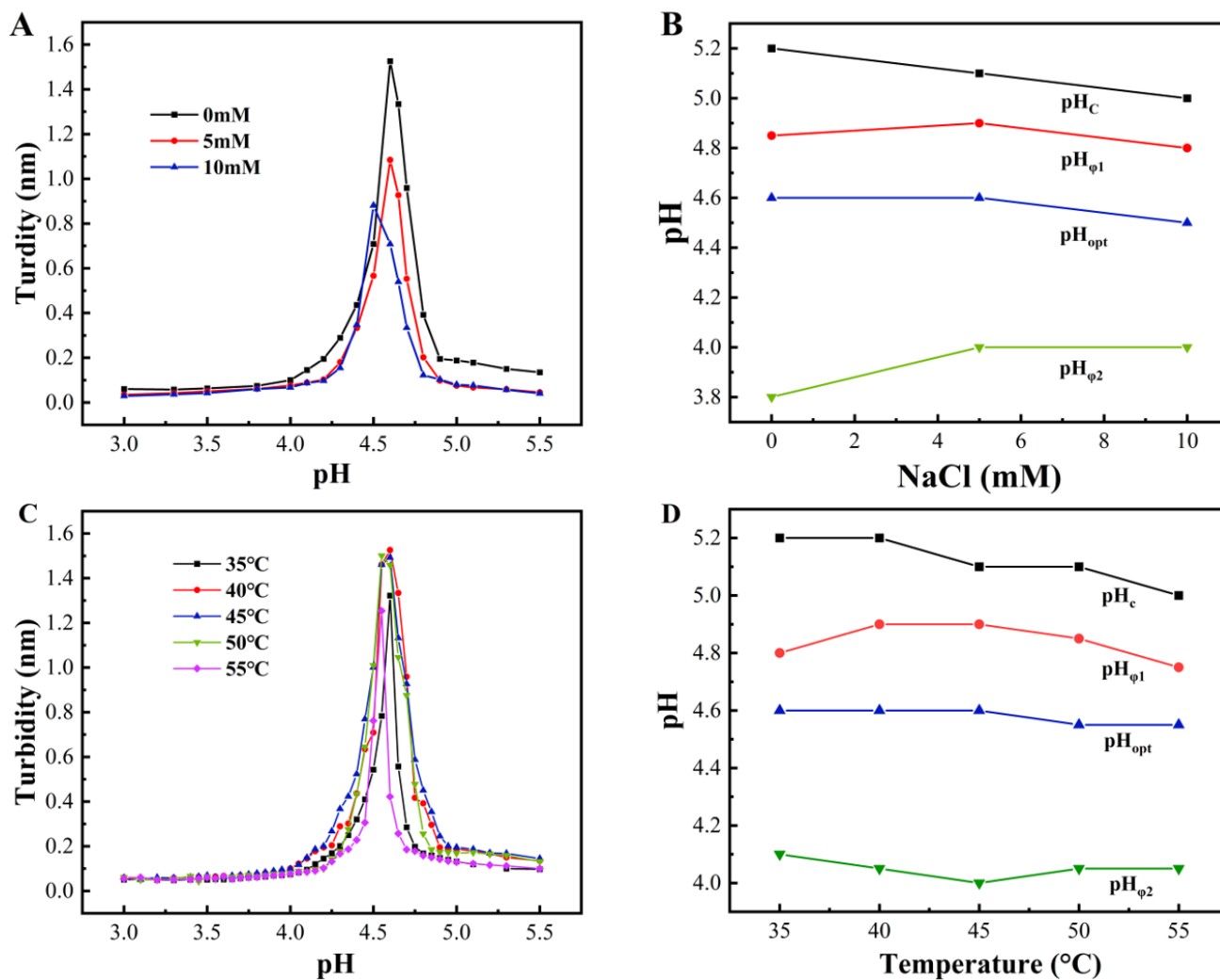


Fig. 3. Turbidity results of GE-CMS mixtures at different C_{NaCl} (A) and different temperatures (C); critical pH values according to the sodium chloride concentration (B) and the temperature (D) of GE-CMS mixtures.

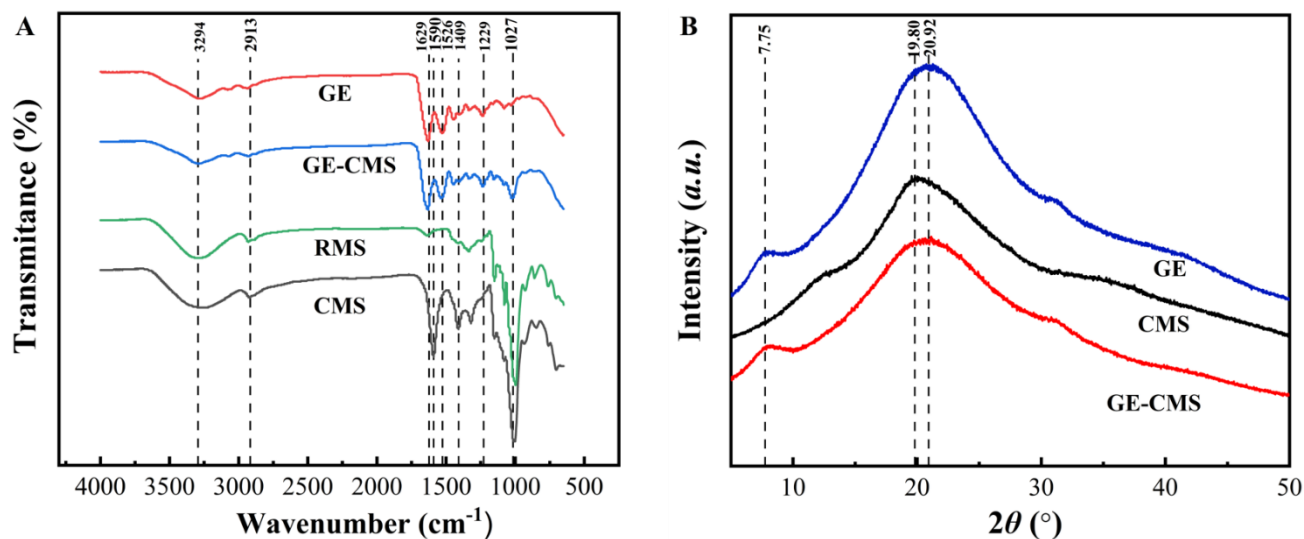


Fig. 4. FT-IR spectra of RMS, CMS, GE, and GE-CMS coacervates (A); and XRD patterns of GE, CMS, and GE-CMS coacervates (B).

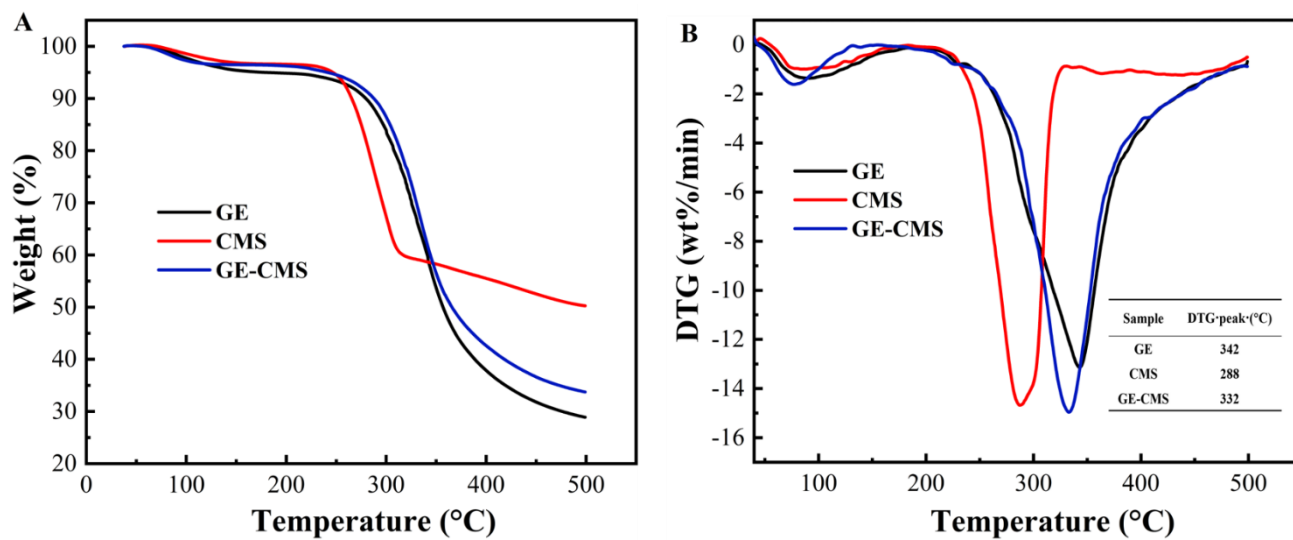


Fig. 5. TGA thermograms of GE, CMS and GE-CMS coacervates.

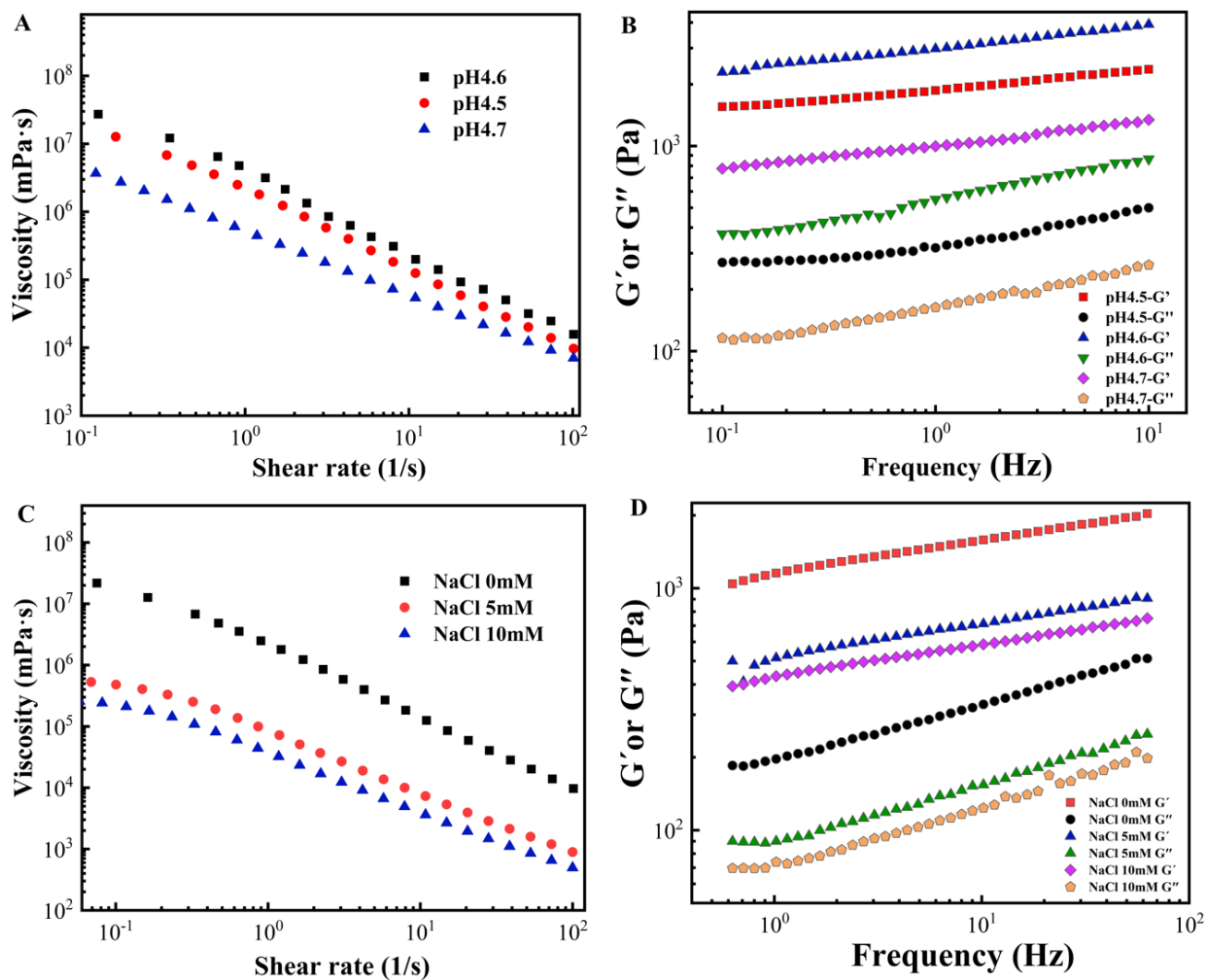


Fig. 6. Viscosity curves and frequency sweep results of GE-CMS coacervates at different pH (A/B) and different C_{NaCl} (C/D).