



Multi-Modal Digital Impressions For Palatal Defects

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1 **Introduction**

2 Head and neck cancer is the 8th most common cancer in the UK affecting males more than
3 females (1). Treatment for head and neck cancer (HNC) may include surgery, chemotherapy,
4 radiotherapy, or a combination of these modalities (2, 3). Treatment for HNC is coordinated
5 via multi-disciplinary teams (MDT) including surgeons, clinical oncologists, pathologists,
6 restorative dentists, radiologists, clinical specialist nurses, speech and language therapists,
7 dieticians, etc. (4-6). As part of surgical intervention, patients may undergo partial or
8 complete maxillectomies which can result in palatal defects; that may either be sealed with
9 composite flaps or left open, thus leaving a palatal defect in the oral cavity (2). The non-
10 surgically sealed defects can be sealed with an obturator prosthesis, sealing the oral passage
11 from the nasal cavities, which aids with speech, swallowing, restores function, and aesthetics
12 (7). Nevertheless, provision of an obturator can be complex as making impressions of the
13 defects can be challenging, and uncomfortable for patients (8).

14

15 Patients who had received radiotherapy can also have post-operative radiation induced
16 trismus with gradual loss of mouth opening (9-11). Normal mouth opening is defined as 40
17 mm of inter-incisal mouth opening measured from the upper left central incisor to the lower
18 left central incisor tooth (or other teeth if the central incisors are not present). Making
19 conventional impressions in patients with trismus can be difficult, and although intra-oral
20 scanners (IOSs) show a high level of accuracy and reduction of trauma to the surgical site (12),
21 the scanner head can be bulky and cannot always be used in such patients, making it
22 challenging to capture the anatomy of the palatal defect. A study used DICOM files from Cone
23 Beam Computed Tomography (CBCT) to take impressions of the palatal defects with
24 promising results (13) . These methods can be utilised to take multi-modal impressions of

25 patients with palatal defects where making conventional impressions may not be possible
26 due to a history of trismus. Surface matching software can be utilised to create composite
27 casts of patients' palatal defects where it is not possible to take impressions using a single
28 modality. The aim of this *in vitro* study was to explore limitations and benefits of digital tools
29 (intra-oral scanning and cone beam computed tomography) to create composite digital casts
30 to capture the anatomy of palatal defects in cases of simulated trismus and compare these
31 composite casts to the gold-standard impressions. The objectives were:

- 32 1. To measure limitations of intra-oral scanning in capturing the maxillary dentition and
33 palatal defect at a range of mouth openings simulating trismus, and
- 34 2. To measure the accuracy which constitute trueness and precision of 3D-printed
35 composite models made by combining CBCT, IOS, and gypsum casts, compared to the
36 gold standard (gypsum casts).

37

38 The null hypotheses were:

- 39 1. There would be a correlation between the amount of data captured of a palatal defect
40 and maxillary dentition with an IOS at different mouth openings simulating trismus,
- 41 2. There would be no statistically significant differences in overall mean precision
42 measurements between composite digital casts compared to the gold standard,
- 43 3. There would be no statistically significant differences in overall mean linear trueness
44 measurements between composite digital casts compared to the gold standard.

45

46 Materials and Methods

47 Capturing Tooth and Soft Tissue Data by an Intra-Oral Scanner at Different

48 Mouth Openings

49 A master model with a cleft palatal defect (**Error! Reference source not found.**) was mounted
50 on a Dentatus semi-adjustable articulator against an opposing fully dentate model. The
51 master model was scanned three times at eight inter-incisal mouth openings (5mm, 10mm,
52 15mm, 20mm, 25mm, 30mm, 35mm, and 40mm) using a 3M™ True Definition Intra-Oral
53 Scanner (IOS). The master model was lightly and evenly coated with 3M™ High Resolution
54 Scanning Spray (3M™ ESPE) as per the manufacturer's instructions prior to scanning.
55 Additionally, the master model was scanned once unmounted using the same IOS, and this
56 scan served as a reference scan. Each scan was exported as a stereolithography (STL) file. Each
57 of the three scans at each inter-incisal opening was imported into Geomagic™ Control 2014
58 (Geomagic® Control, 3D Systems Inc, Darmstadt, Germany) and, following a best-fit iterative-
59 closest point (ICP) alignment, all three were merged to create a composite file for each mouth
60 opening. Amount of data capture was measured by superimposing each composite scan (5,
61 10, 15, 20, 25, 30, 35, and 40 mm) against the scan of the master model to measure data loss
62 (loss of triangles/polygons captured) at each mouth opening compared to the master model.
63 Data was measured as percentage coverage of each experimental cast at each mouth opening
64 superimposed against the scan of the master model.

65

66 **Fabrication of Composite Models Combining Cone-Beam Computed**
67 **Tomography with Digitised Gypsum Casts or Intra-Oral Scanning**

68 Five impressions of the master model were taken using 2 mm spaced special trays and using
69 a three-consistency/two-step impression technique with heavy, medium, and light bodied
70 polyvinyl-siloxane (PVS) following manufacturer's instructions. Impressions were cast in type
71 IV gypsum according to the manufacturer's instructions. The 5 gypsum casts were scanned
72 using a 3Shape™ R700™ laboratory scanner and were exported as STL files. The experimental
73 protocols are shown on **Error! Reference source not found.**. The master model was scanned
74 five times each using the following techniques: **Planmeca ProMax 3D Mid® Cone-Beam**
75 **Computed Tomography** (CBCT-P) (field of view (FOV) of 80x80mm, 90 kilovolt (kV) x 2
76 milliamperere (mA), and exposure time of 20 seconds). DICOM files were converted into STL
77 files; **Accuitomo 170® Cone-Beam Computed Tomography** (CBCT-A) (FOV of 80x80mm size,
78 60 kV x 1 mA, and exposure time of 17.5 seconds). DICOM files were converted into STL files;
79 **3M™ True Definition IOS Intra-oral Scanner** (IOS-T); **Planmeca PlanScan® IOS Intra-oral**
80 **Scanner** (IOS-I). Data from the 5 scans were exported as STL files.

81

82 Data acquired from scanning of master model using the four digital techniques and the
83 scanning of the gypsum casts were combined using Geomagic® Control 2014™ to create 30
84 composite files (5 each of: CBCT-P/IOS-T; CBCT-P/IOS-I; CBCT-P/Gypsum; CBCT-A/IOS-T;
85 CBCT-A/IOS-I; CBCT-A/Gypsum). The 30 composite files were 3D-printed using an Objet 260®
86 Connex1 (Stratasys®, San Francisco, USA) 3D-printer of 16-micron layer resolution using
87 translucent composite resin (RGD720) with support resin (SUP705). The support resin was
88 removed, and the models cleaned with Genie 400 jet wash machine (Gemini Cleaning Systems

89 Ltd) to remove support resin from the models. Each of the thirty 3D-printed composite
90 models, five gypsum models, and the master model were scanned using a 3Shape™ R700™
91 laboratory scanner and exported as STL files. The trueness and precision of models produced
92 from each of the techniques (6 digital and 1 conventional) were compared to scans of the
93 master model.

94

95 **Measuring Trueness and Precision of The Composite Models**

96 The STL files from each of the 30 composite models and 5 gypsum models were imported into
97 Geomagic Control 2014™. Each scan was digitally superimposed to the scan of the master
98 model using an initial best-fit alignment based on an ICP algorithm using 300 iterative pairs
99 of points, before a more precise fine-superimposition was performed using 1500 pairs of
100 points. Trueness was determined using the 3D-Compare function we obtained a heat map
101 representing 3D-deviations (μm) on the X, Y, and Z axes of the experimental datasets
102 compared to the scan of the master reference model within $\pm 3\text{mm}$ (**Error! Reference source**
103 **not found.a**). Blue indicated negative deviations, red indicated positive deviations, green
104 showed no deviations, and grey represented missing data.

105

106 The Target Point function was used to set a total of 180 points to analyse linear deviation. The
107 target points were placed on the master reference model which allowed measuring the same
108 locations across all superimpositions (**Error! Reference source not found.b**). Average linear
109 deviations in the X, Y, and Z axes were measured across the 180 points for each of the
110 superimpositions. Lower deviation values indicated higher trueness.

111

112 Precision of each of the techniques was measured using previously published methods which
113 utilised best-fit alignment algorithm on Geomagic® Qualify 11 surface metrology software
114 (Geomagic® Incorporated, North Carolina, USA)(14). Each individual model scan was digitally
115 superimposed against each of its counterparts using Geomagic Control 2014™ using similar
116 methodology described above. Differences between each technique was assessed by
117 measuring average differences on the X, Y, and Z axes for each superimposition/technique.
118 Differences between each superimposition were thus related to manufacturing and
119 processing error for each technique as individual casts from each experimental arm and the
120 control were produced in the same manner. The technique with the lowest mean
121 measurement was the most precise.

122

123 **Statistical Analyses**

124 Data was tabulated into a spreadsheet and was classified per technique and mouth opening.
125 Statistical analysis was done using Statistical Package for Social Science SPSS 27.0 (IBM Corp.
126 Released 2020. IBM SPSS Statistics for Macintosh, Version 27.0. Armonk, NY: IBM Corp).
127 Pearson Correlation Coefficient was used to assess the correlation between mouth opening
128 (mm) and percentage (%) coverage between the master model and the composite models at
129 each mouth opening (5mm, 10mm, 15mm, 20mm, 25mm, 30mm, 35mm, and 40mm).
130 Trueness data for the composite casts was not normally distributed and is described in
131 median (mm) and Inter-Quartile Range [IQR]. Kruskal-Wallis and post-hoc Wilcoxon rank-sum
132 tests were used to measure differences in trueness between the 6 experimental groups and
133 the control. The smallest median value indicated the technique of highest trueness. Precision
134 data conformed to a normal distribution and therefore was computed using mean (mm) and

135 SD from the repeated superimpositions of each technique. The smallest mean value indicated
136 the most precise technique. Univariate Analysis of the Variance (ANOVA) and post-hoc
137 Bonferroni tests were used to assess differences in precision between the 6 experimental
138 groups and the control. Statistical significance was inferred where $p < 0.05$.

139

140 **Results:**

141 **Mouth Opening**

142 Data for mouth opening showed that as mouth opening decreased, data captured by the 3M™
143 True Definition intra-oral scanner also decreased. **Error! Reference source not found.** shows
144 the percentage coverage from each composite scan against the master model at each mouth
145 opening. The results plateaued at 35 mm with only a slight increase in percentage coverage.
146 At 40 mm, the percentage coverage of the scan decreased to the level of 25 mm mouth
147 opening. Pearson Correlation Coefficient (r) was 0.93, showing a strong positive correlation
148 between increased mouth opening and increased data capture ($p = 0.0010$). Each composite
149 scan was analysed individually against the master reference to evaluate the deficient areas at
150 each mouth opening. At ≥ 20 mm inter-incisal opening, the intra-oral scanner was able to
151 capture all the relevant data (tooth and palatal level) to aid in the fabrication of an obturator
152 prosthesis. At 15 mm and below, there were limitations in capturing tooth and soft tissue data
153 which would compromise use of IOS. Table 1 shows results of qualitative analysis capturing
154 tooth and soft tissue data.

155

156 **Trueness of The Composite Models:**

157 Median and Inter-Quartile Ranges (IQR) are shown on Table 2. The composite models with
158 highest trueness were, in order: Accuitomo CBCT (A) + True Definition IOS (T) > Planmeca
159 CBCT (P) + True Definition IOS (T) > Accuitomo CBCT (A) + gypsum casts (G) > Planmeca CBCT
160 (P) + gypsum casts (G) > Planmeca CBCT (P) + PlanScan IOS (I) > Accuitomo CBCT (A)+ PlanScan
161 IOS (I) > And the gypsum casts had the lowest trueness (G). Kruskal-Wallis and post-hoc
162 Wilcoxon rank-sum tests showed statistically significant differences between the six
163 composite models compared to the gypsum models, indicating that all digital composite
164 models had higher trueness compared to the gypsum models ($p<0.001$).

165

166 **Precision of The Composite Models:**

167 Mean and [Standard Deviation] measurements are shown on Table 3. The most precise
168 composite models were, in order: Accuitomo CBCT (A) + True Definition IOS (T) > Planmeca
169 CBCT (P)+ True Definition IOS (T) > Accuitomo CBCT (A)+ gypsum casts (G) > Planmeca CBCT
170 (P)+ gypsum casts (G) > Accuitomo CBCT (A)+ PlanScan IOS (I) > Planmeca CBCT (P)+ PlanScan
171 IOS (I) > And the least precise group were the gypsum casts (G). Univariate Analysis of
172 Variance (ANOVA) and post-hoc Bonferroni tests indicated statistically significant difference
173 between the six composite models compared to gypsum models ($p<0.001$) suggesting that
174 the composite models were more precise compared to gypsum models.

175

176 **Discussion**

177 All null hypotheses were rejected. This study assessed the suitability of CBCT and IOS to
178 fabricate models suitable for obturators for palatal defects patients. The results confirmed

179 the limitations of intra-oral scanning in patients with reduced inter-incisal distance and
180 suggest a fresh rethink on how to achieve accurate impression taking on this cohort of
181 patients by potentially harnessing other digital techniques, such as CBCT scanning. The
182 composite 3D-printed digital models can potentially be used clinically as the differences
183 compared to the master reference model were within acceptable clinical values. Additionally,
184 the composite models were more precise and had higher trueness than the gold-standard
185 gypsum casts. To our knowledge, this *in vitro* study was the first to explore in detail the
186 trueness and precision of combined digital techniques for model fabrication. Rehabilitation
187 of patients with head and neck cancer or trismus requires a degree of innovation and
188 creativity therefore, using composite models to deliver clinical care to patients could help
189 deliver prosthesis for patients who would otherwise be unable to have impressions taken.

190

191 Medical imaging systems such as CBCT are being used as an alternative to conventional
192 impressions to capture the anatomic detail of the maxillectomy defect and surrounding
193 tissues in HNC patients. CBCT is capable of providing accurate radiographic and volumetric
194 data which can be used in the construction of digital impressions (15); however, their accuracy
195 in capturing the oral soft tissue and dentition is generally sub-optimal due to low contrast
196 resolution yielded by the oral soft tissues, scattering radiation and beam-hardening artifacts
197 caused by dental restorations (16). This limitation can be resolved by utilising digital scans
198 from intra-oral scanners as they can provide scatter-free, high-resolution data of the oral soft
199 and hard tissues and dental restorations.

200

201 Intra-Oral Scanners have been reported as accurate and reliable to digitally record partially
202 or completely edentulous arches with maxillectomy defects (17, 18). Although technique

203 sensitive, once the scan was obtained there is no risk of distortion thus eliminating a
204 multitude of errors and in return improving patient pathway and experience. Furthermore,
205 previous studies have demonstrated that intra-oral scanning of single teeth, sextants and
206 quadrants are more accurate than conventional impression techniques (19-22). On the other
207 hand, different inferences exist in the literature for full-arch scans (23-29). The accuracy of
208 intra-oral scanners tends to decrease as the area of scanned oral surface increases due to the
209 device's image stitching process that may lead to propagation of errors and therefore a
210 distortion of the real anatomy. IOSs and their technologies are constantly revised and
211 updated, and improvements in accuracy are inevitable as manufacturers update hardware
212 and improve the acquisition software.

213

214 The results of this study suggested that the use of intra-oral scanners may not be possible in
215 patients with mouth opening <20 mm. It would thus be a sensible proposal to carry out an
216 intra-oral scan of every patient about to undergo resective surgery for head and neck cancer.
217 If the patient then develops trismus due to surgical resections or post-operative radiotherapy,
218 a CBCT can be taken post-operatively. The CBCT can capture the soft tissue anatomy and
219 defect, whereas the dentition can be captured using IOS. The CBCT and IOS can then be
220 combined to create a composite model which can be utilised to deliver a prosthesis to these
221 patients without the need for conventional impressions.

222

223 For convenience we used a single intra-oral scanner (3M True Definition, 3M, ESPE) to assess
224 data capture at different mouth openings. Although the resolution and accuracy among
225 different intraoral scanners can vary, 3M™ True Definition IOS has been extensively
226 investigated in the literature and is considered amongst the best performing IOSs in terms of

227 resolution, trueness, and precision (30-34). One advantage of using this scanner is its notably
228 smaller tip size (254 x 16.2 x 14.4 mm) compared to other commercially available IOS. The
229 results above demonstrate that if mouth opening is less than 20 mm, the use of an intra-oral
230 scanner is not advocated due to the lack of clinical information captured. In such cases,
231 composite models may be used to allow the construction of an obturator prostheses.

232

233 This study showed that the digital techniques were truer and more precise compared to the
234 gypsum casts. Although gypsum casts are considered the gold standard in prosthodontics,
235 they are labour-intensive and depend on operators' skills for precision. Impression materials'
236 properties, handling, thickness, and polymerisation shrinkage as well as gypsum mixing,
237 pouring and setting expansion can introduce errors in models including voids, drags, and lost
238 detail (35). The trueness and precision of gypsum models depended on the impression
239 materials' properties, type of tray, gypsum material's properties, and bubbles/drags which all
240 contributed to the lower accuracy in this experiment. Conventional impressions were found
241 to experience dimensional changes through thermal contraction from mouth to room
242 temperature reaching 0.068-0.088mm posteriorly and 0.040-0.052mm anteriorly in clinical
243 settings (35). Dental gypsum casts have been shown to exhibit a linear setting expansion of
244 0.14 – 0.35% after 120 hours (36).

245

246 Compared to the 3M™ True Definition IOS, the PlanScan® intraoral scanner showed inferior
247 trueness and precision. This may be related to the different optical technologies utilised by
248 each IOS to capture the surface morphology. True Definition uses active wavefront sampling
249 technology, whilst PlanScan® uses laser triangulation. Our results agree with other studies.
250 Mennito et al 2019 assessed the trueness and precision of full arch maxillary digital

251 impressions of a human cadaver, and reported that the PlanScan® was significantly less
252 accurate than other intra-oral scanners (37). Kim et al 2021 also reported greater accuracy of
253 a 3M™ True Definition IOS compared to PlanScan® IOS (38).

254 In an *in vivo* study on 12 maxillectomy patients, (13) 3D-printed models made from CT
255 scanners (Optima CT520Pro) and intra-oral scanning were reported to be as true and precise
256 as gypsum models with no statistically significant difference in linear deviations between the
257 digital and conventional models. The authors used the composite 3D-printed models to
258 fabricate conventional cobalt chrome obturator prostheses and reported a good fit around
259 the rest seats and minor connectors (13). This is an area we will investigate in the future.

260

261 The results of this *in vitro* study may differ from the clinical situation as the accuracy of models
262 may be influenced by the presence of anatomical structures, saliva, limited space, and patient
263 movement. Also, the surface optical properties, morphology and chemical composition of the
264 master reference model used were different from the intra-oral situation. Moreover, the use
265 of a CBCT scanner in a clinical situation may yield different results since soft tissues and teeth
266 may scan differently compared to an *in vitro* experiment. The combination and manipulation
267 of scans on Geomagic® Control 2014™ was straightforward in our study but the situation may
268 be different in a clinical scenario where there are fewer areas in common between scans to
269 allow superimposing the files. Furthermore, the benefits of using CBCT scanning as an
270 impression technique clinically must be weighed against the risks of exposure to ionizing
271 radiation.

272

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