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ToFFi – Toolbox for frequency-based fingerprinting of brain signals

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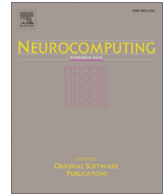
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Original software publication

ToFFi – Toolbox for frequency-based fingerprinting of brain signals



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ABSTRACT

Spectral fingerprints (SFs) are unique power spectra signatures of human brain regions of interest (ROIs, Keitel & Gross, 2016). SFs allow for accurate ROI identification and can serve as biomarkers of differences exhibited by non-neurotypical groups. At present, there are no open-source, versatile tools to calculate spectral fingerprints. We have filled this gap by creating a modular, highly-configurable MATLAB Toolbox for Frequency-based Fingerprinting (ToFFi). It can transform magnetoencephalographic and electroencephalographic signals into unique spectral representations using ROIs provided by anatomical (AAL, Desikan-Killiany), functional (Schaefer), or other custom volumetric brain parcellations. Toolbox design supports reproducibility and parallel computations.

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1. Introduction

Brain dynamics and brain oscillations are among the most important topics in neuroscience. Different methods proved to be useful for studying robust whole-brain, as well as regionally-specific patterns of activity, called brain fingerprints. They can serve as signatures for mental states during task execution or rest [1–4]. The frequency of oscillations turned out to be one of the key features in many studies describing particular regions of interest (ROIs) [5–7] and large-scale brain networks [8–12].

It is important to note that previously the term *brain fingerprinting* was mainly associated with forensic science and biometry. In forensic sciences, brain fingerprinting was the name of the procedure of extracting event-related potentials characteristic for the situation where during an interrogation a suspect was confronted with concealed information relevant to a crime scene in which he was potentially involved [13–15]. The name is an analogy to traditional methods of recovering specific marks left on a surface by friction ridges of a human finger that aims to identify people

involved in a criminal event. In biometry, several neuroimaging-based approaches were designed to extract features unique for a given person [16–24].

Starting from the 2000s, another meaning of brain fingerprinting has been emerging. Researchers started to think about fingerprints of neuronal interaction dynamics, leaning towards network neuroscience and spectral methods. They wanted to test if it is possible to find markers of various cognitive processes [25,2,1,3], brain diseases [26,27], brain areas or networks [28–34,7].

In this spirit, some reviews proposed frameworks for capturing the specificity of cortical dynamics using term *spectral fingerprints* [35,5,36]. Shortly after, Keitel and Gross defined this term strictly by proposing a first formalized pipeline for Spectral Fingerprinting that is central in our work [7,27].

Spectral fingerprints (Fig. 1) defined by Keitel and Gross [7] play a role as biomarkers that are sufficiently specific to permit the successful identification of brain regions using their spectral characteristics. Moreover, spectral profiles' peaks that correspond to the natural frequencies of ROIs [12,37], are consistently modulated by specific tasks, neurological or mental disorders. They can be generalized across groups of participants [27,7]. In this paper, we

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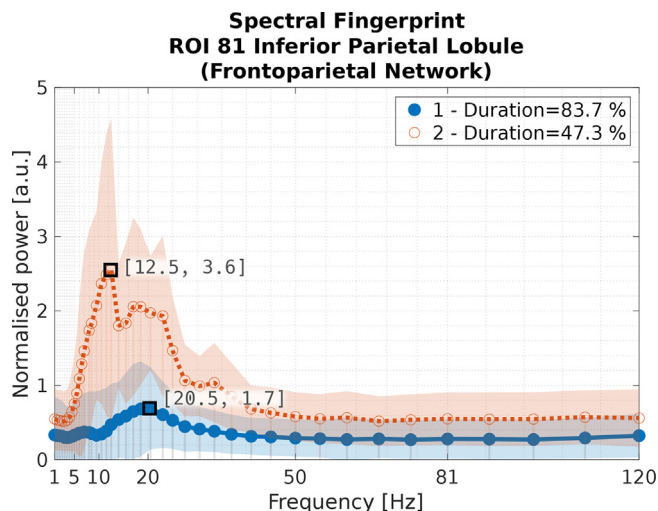


Fig. 1. A spectral fingerprint of the inferior parietal lobule. For this particular region, it consists of two spectral modes. It is formed by clustering power spectra segments (normalized, i.e. spectral power in comparison to the whole brain) first on the individual subjects level and then clustered again on the group level. Each mode corresponds to one of the centroids found by the clustering algorithm. Shaded regions depict the standard deviation (1σ) estimated from the covariance matrix of the Gaussian Mixture Model component corresponding to the given spectral mode. The first mode peaks at 12.5 Hz, and the second mode peaks at 20.5 Hz. The frequency axis resolution can be set to logarithmic to optimize spectral analysis resolution of lower frequencies. Duration is shown as a percentage of time segments in which each spectral mode was present on average during recording.

introduce a novel implementation of the Spectral Fingerprinting technique, in a highly configurable MATLAB toolbox.

2. Problems and background

There are many open software packages available to analyze neural data. The Fieldtrip Toolbox¹ [38] was designed to perform analysis both on sensor and source level of EEG/MEG/iEEG/NIRS data. EEGLAB² [39] helps with processing continuous and event-related electrophysiological data implementing many analytic methods (ICA, time/frequency analysis, artifact rejection, event-related statistics, microstates analysis) and several useful routines for visualization. To simulate brain dynamics, perform connectivity analyses, and solve forward/inverse problems, the supFunSim³ toolbox [40] and the Virtual Brain⁴ system [41] are among suitable choices. However, there is no open software specifically for constructing and analyzing spectral fingerprints, and our work attempts to fill this gap. We designed the Toolbox for Frequency-based Fingerprinting (ToFFi, https://github.com/mic-holeodon/ToFFi_Toolbox) for analysis of MEG, EEG, and other multichannel data. Users can configure many parameters for each stage of processing, including the selection of the brain parcellation, and decide which of them will run in parallel (cluster computations are supported). Results of the calculations are reproducible thanks to the implemented control using pseudo-random number generators and visualization scripts. Currently, none of the already available toolboxes is similar to ToFFi.

ToFFi was not designed as a generic MEG/EEG signal processing suite or a collection of conventional processing methods. ToFFi's sophistication builds upon an interplay between spectral methods, spatial filtering, and clustering that together serve a specific pur-

pose – the construction of spectral fingerprints for individual brain regions. Coupled with the great research promise that Spectral Fingerprinting brings to brain research, we have released ToFFi for the benefit of a wider neuroscientific community.

3. Software framework

3.1. Software architecture

ToFFi is a modular piece of software that allows multichannel data preparation, spectral fingerprint construction and analysis, and visualization of the results (Fig. 2). It consists of five components: I. Data Preparation, II. Spectral Fingerprinting, III. Analysis, IV. Presentation, and V. Maintenance (Fig. 3). The Data Preparation module (I) is responsible for arranging sensor time series signals, spatial filters, and brain parcellation data, for processing by the second step routines. The Spectral Fingerprinting (II) module transforms MEG/EEG multichannel array of signals, through a series of five stages, into spatially localized power spectrum-driven representations called spectral fingerprints (Fig. 4). Fourier Transform, source reconstruction (beamforming), and Gaussian Mixture Modeling algorithms are used to compute spectral fingerprints both at the individual and the group level. The third component (III) consists of additional routines that can analyze particular output files from component II. Currently, we have implemented group-level brain regions identification, individual-level brain regions identification, and regional clustering (network analysis) - all based on the concept of modeling brain activity as spectral fingerprints. The Presentation component (IV) is a collection of auxiliary scripts used to visualize particular results of performed computations for easier interpretation. Maintenance routines (V) are used to automate some parts of the workflow, e.g.: manage configuration files, manage output data files, etc. A more detailed description of how the data are transformed can be found in Appendix A (6. METHODS), Fig. 5, Fig. 6, and Fig. 7, which summarize the whole pipeline.

3.2. Software functionalities

Spectral Fingerprinting can be performed on multichannel time series data (e.g. MEG, EEG) of arbitrary size, with any sampling-frequency adjusted to the desired frequency resolution, acquired from a single or multiple subjects, and divided into segments of selected, equal duration (e.g. 1000 ms). These segments may contain non-overlapping pieces of a continuous recording (e.g. resting-state) or trials with brain responses for several repetitions of the same experimental condition (event-related paradigm). For individual-level analysis, the toolbox offers a reconstruction of voxel-wise time series power spectra with beamforming using pre-computed spatial filters (e.g. LCMV, [42,43]) and multichannel empirical sensor signals or artificial white Gaussian noise signals. Power spectra of ROIs can be estimated both at individual and group level, using different brain parcellations (anatomical: AAL [44], Desikan-Killiany [45]; functional: Schaefer [46]), and optionally normalized. These spectra can be clustered (currently, only the k-means algorithm is implemented) with arbitrary distance metric and subsequently modeled as a regularized Gaussian mixture of regional spectra with a fixed or optimal number of clusters to construct group-level fingerprints. The user can also estimate the accuracy of identification of brain regions from their spectral fingerprints using cross-validation. Hierarchical clustering of spectral fingerprints (network analysis) was also implemented. The scope of selected brain regions of interest (ROIs) and set of subjects of choice can be limited if desired. For the majority of stages, one

¹ <https://www.fieldtriptoolbox.org/> accessed: 04.05.2023

² <https://eeglab.org/> accessed: 04.05.2023

³ <https://github.com/nikadon/supFunSim> accessed: 04.05.2023

⁴ <https://www.thevirtualbrain.org/> accessed: 04.05.2023

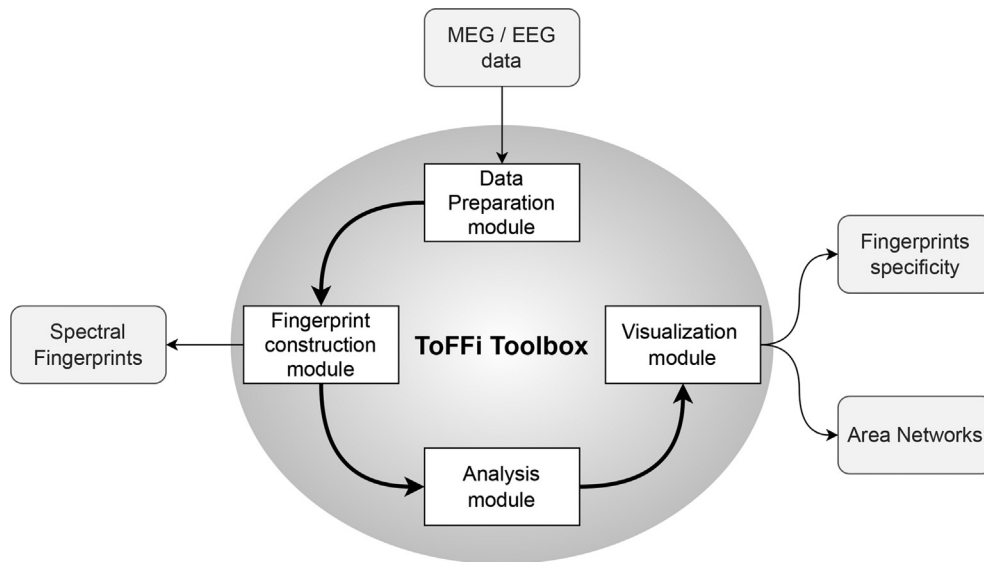


Fig. 2. Compact schematic of the ToFFi Toolbox.

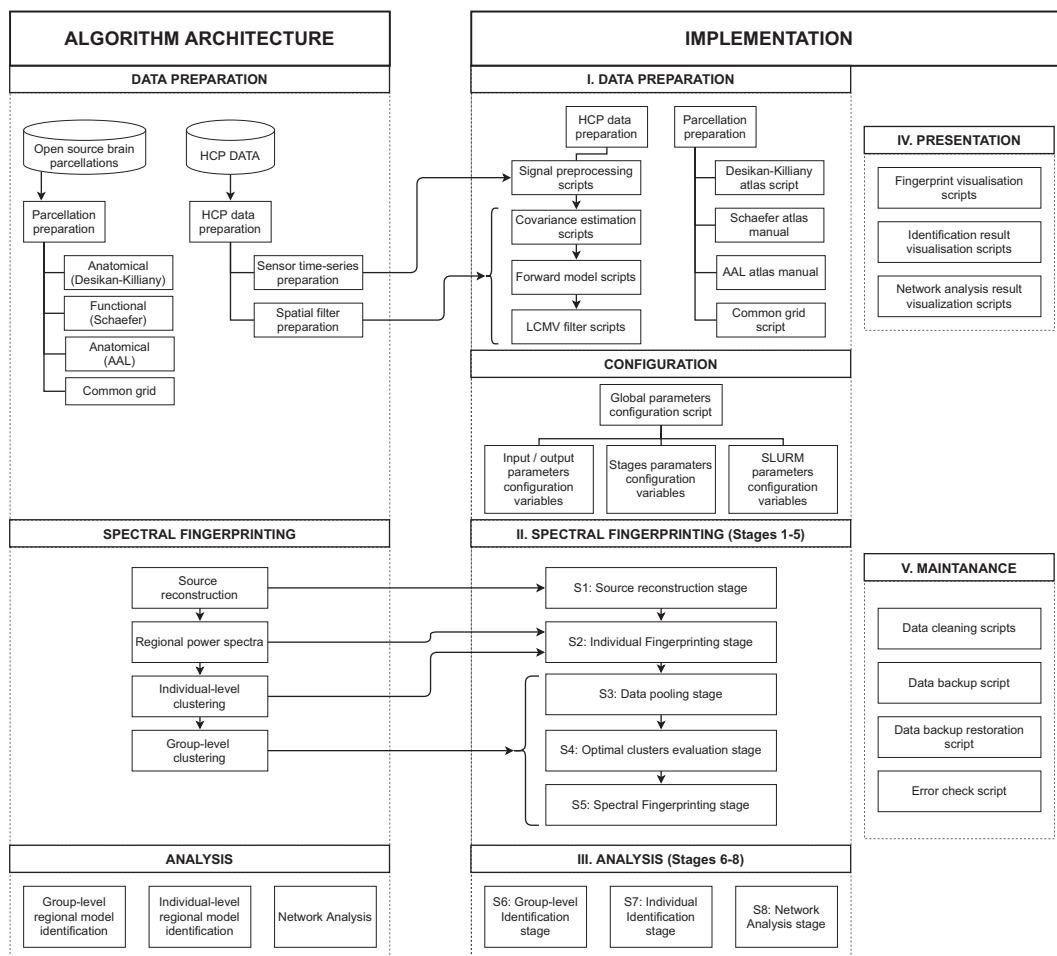


Fig. 3. ToFFi toolbox architecture.

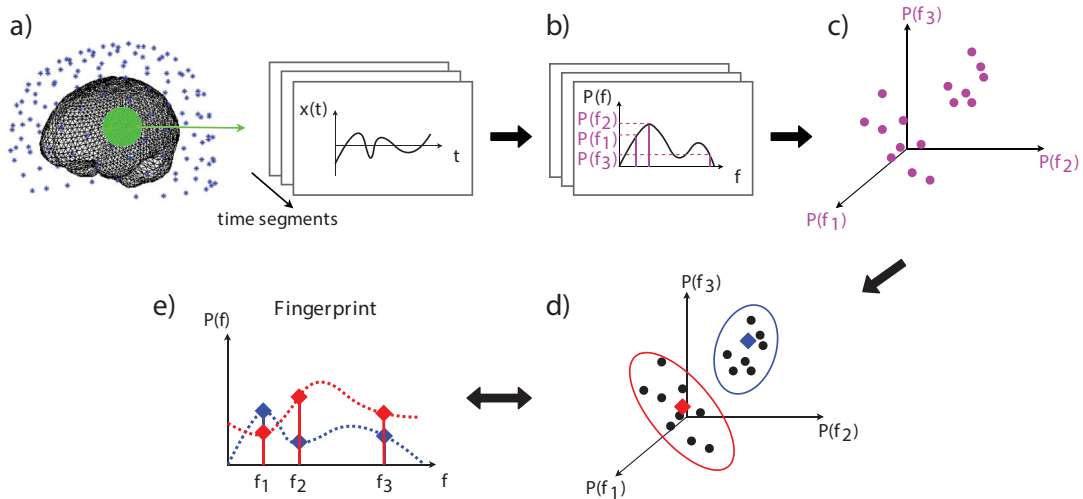


Fig. 4. Illustration of the Spectral Fingerprinting algorithm [7]. a) Mean-field, electrical activity of the brain is recorded via an array of sensors (blue dots). A beamformer [43] solves so-called *inverse problem*, thus enabling reconstruction of the source activity in selected voxels constituting chosen brain regions of interest (green area). Source-level time series are cut into segments of equal length. b) Power within each segment is estimated for a given set of frequencies of interest (here three frequencies, f_1, f_2, f_3 , are shown for readability) and then averaged across locations inside the region of interest. c) Power spectrum of each segment is represented as a point in a n -dimensional frequency space, where power of the selected frequencies provides coordinates of the point. d) Segments are clustered together. Each centroid is equivalent to one *spectral mode* of a given brain region and depicted as an interpolant curve spanned between the frequencies of interest in the resulting fingerprint (interpolation type is arbitrary, as it serves visualization purpose only).

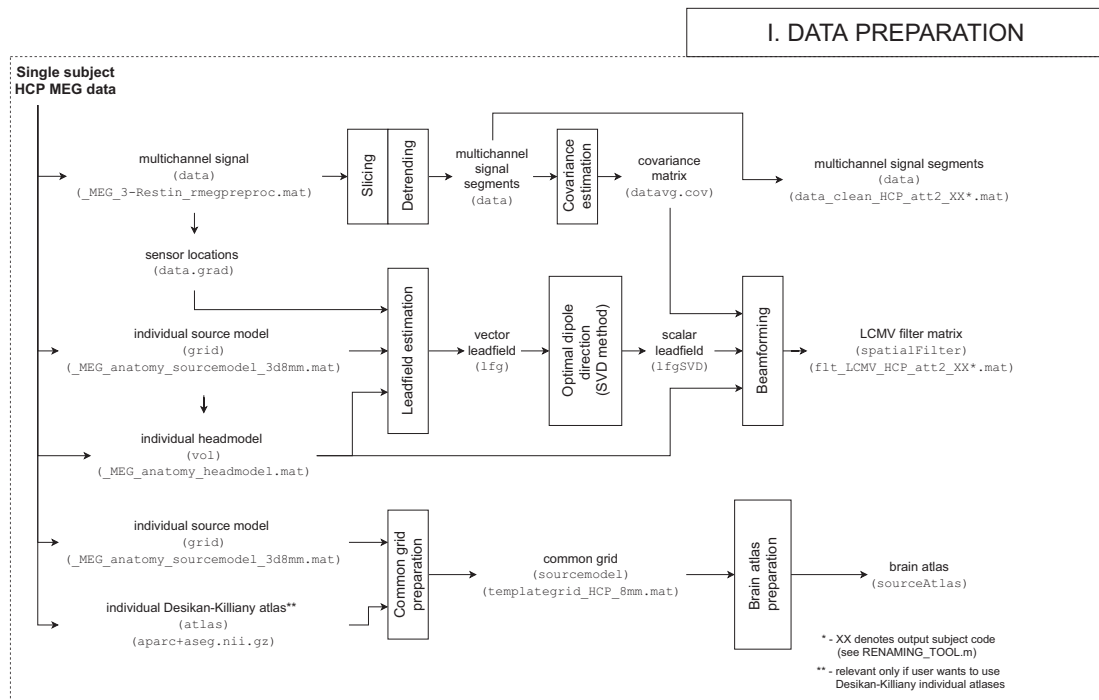


Fig. 5. Diagram of how the data are processed by the DATA PREPARATION component (see Fig. 3). Each depicted piece of data is endowed with its name, MATLAB workspace variable name (middle parentheses), and a file name (bottom parentheses) if it is read or written to the disk during processing.

can perform computations in parallel on a single computer with multiple cores, or on a grid of multiple-core machines orchestrated via workload manager (currently, only SLURM manager is supported). Interpretation of the outputs of the software components II and III are supported with visualization routines. For reproducibility, data maintenance routines and pseudo-random generator control are implemented as well.

4. Implementation and empirical results

4.1. Implementation

The toolbox can be operated under Linux, macOS, and Windows systems. Maintenance scripts (V) are coded mostly in Bash, which is accessible both for Linux (as default) and Windows (us-

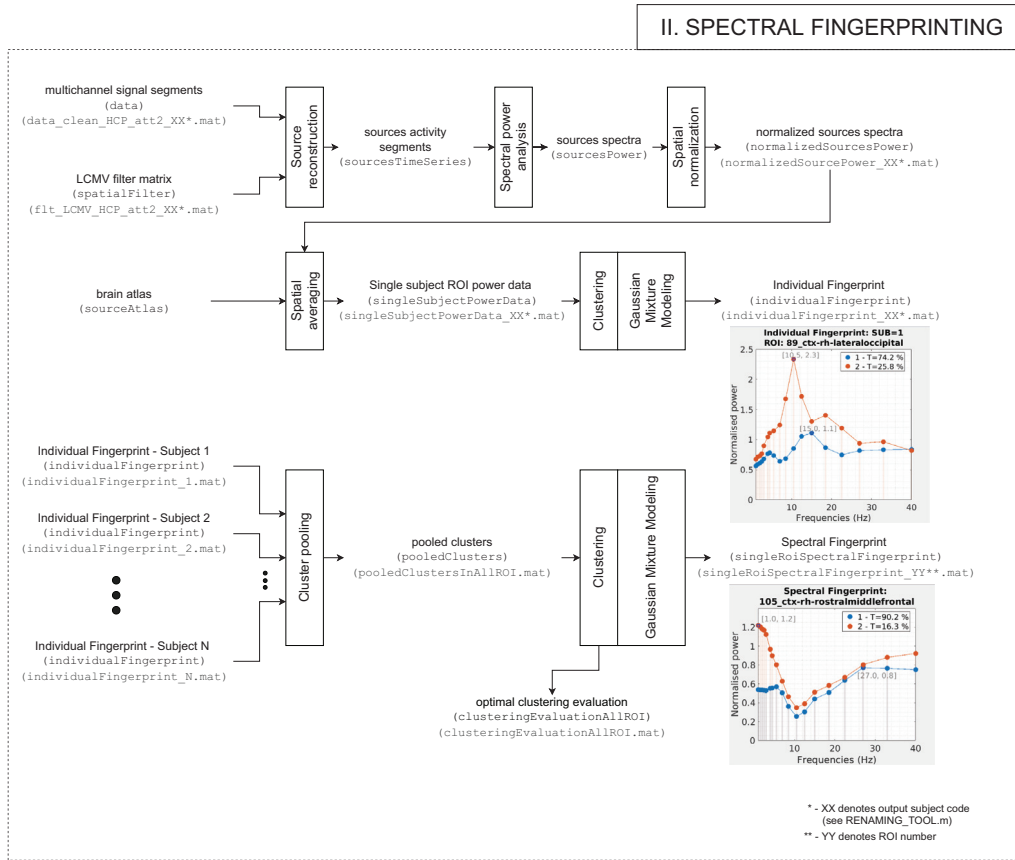


Fig. 6. Diagram of how the data are processed by the SPECTRAL FINGERPRINTING component (see Fig. 3). Each depicted piece of data is endowed with its name, MATLAB workspace variable name (middle parentheses), and a file name (bottom parentheses) if it is read or written to the disk during processing.

ing Cygwin, cmdr, or other shell emulator). All calculations are carried out entirely in MATLAB with Signal Processing Toolbox, Statistics and Machine Learning Toolbox, Parallel Computing Toolbox, and open-source Fieldtrip Toolbox [38]. For compatible versions of MATLAB and Fieldtrip, see Table 1. Additionally, `vline.m` and `hline.m` functions⁵ by Brandon Kuczynski are used for plotting, and `HZmvntest.m` function⁶ by Antonio Trujillo-Ortiz for multivariate normality testing. If the user wishes to enable cluster computations, the toolbox is prepared to work in coordination with the SLURM workload manager⁷. To the best of our knowledge, there is no other software for Spectral Fingerprinting available, apart from the illustrative beta-version script referenced by the authors of [7].

4.2. Empirical results

Keitel and Gross [7] showed that rendering regional brain activity as a combination of spectra via Spectral Fingerprinting allows for the identification of ROIs with high accuracy. They noticed that clustering of the brain areas according to the similarity of spectral profiles shows patterns similar to macroscale organization of the human brain cortex. Auditory spectral profiles turned out to be modulated during auditory processing. Lubinus and colleagues [27] have discovered that visual depriva-

tion is reflected in the modulation of spectral fingerprints, indicating possible correspondence with the structural and functional adaptation of the human brain. Likewise, Mellem with collaborators [6] demonstrated via a similar method that there is a mix of lower and higher frequency peaks across the brain and it does not follow a simple lower order-higher order processing hierarchy.

5. Illustrative example

Please consult the following parts of Appendix A to run Illustrative Example smoothly: *Chapter 2. Conventions* – to learn notation used throughout the documentation; *Chapter 3. Installation* - to set up a computational environment properly, *Sections 5.3 and 5.4* - to get the input data.

After installation, one is advised to follow the instructions in *Chapter 4. Illustrative Example* in Appendix A to complete the illustrative example using the Human Connectome Project MEG dataset (HCP Reference Manual, [47]). We have selected N = 10 subjects with the MEG resting-state cleaned signal acquired via a 248 channel array in three subsequent runs, approximately 3 min each.

Spectral Fingerprinting routines were configured to optimize the frequency resolution for the lower frequencies, thus accounting for the 1/f power trend present in the typical electrophysiological activity of the human brain. The proper number of clusters to be constructed was estimated using the Silhouette optimality criterion. Choosing cosine dissimilarity as a distance measure helped to compose frequency clusters of power spectra similar in shape,

⁵ <https://www.mathworks.com/matlabcentral/fileexchange/1039-hline-and-vline> accessed: 04.05.2023

⁶ <https://www.mathworks.com/matlabcentral/fileexchange/17931-hzmvntest> accessed: 04.05.2023

⁷ <https://slurm.schedmd.com/> accessed: 04.05.2023

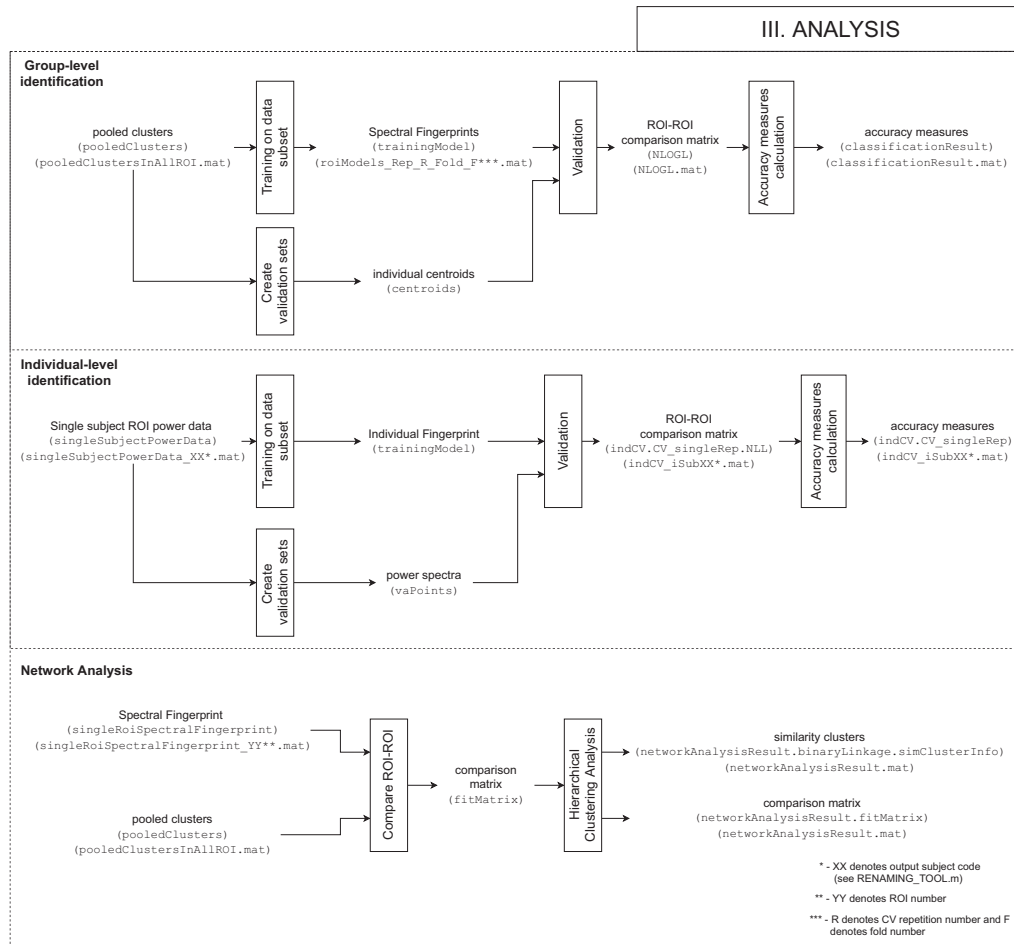


Fig. 7. Diagram of how the data are processed by the ANALYSIS component (see Fig. 3). Each depicted piece of data is endowed with its name, MATLAB workspace variable name (middle parentheses), and a file name (bottom parentheses) if it is read or written to the disk during processing.

Table 1
Software metadata (optional)

Nr.	(executable) Software metadata description	Please fill in this column
S1	Current software version	20211013
S2	Permanent link to executables of this version	https://github.com/micholeodon/ToFFi_Toolbox
S3	Legal Software License	GNU Lesser General Public License v2.1
S4	Computing platform/Operating System	Linux, Microsoft Windows, macOS
S5	Installation requirements & dependencies	MATLAB (R2020a, R2020b, R2021a, R2021b, or R2022a) + Signal Processing Toolbox, Statistics and Machine Learning Toolbox, Parallel Computing Toolbox; Fieldtrip Toolbox version 20210816
S6	If available, link to user manual - if formally published include a reference to the publication in the reference list	https://github.com/micholeodon/ToFFi_Toolbox/tree/master/ToFFi_Toolbox-20211013/docs/ToFFi_Manual.pdf
S7	Support email for questions	michu.kom@gmail.com

diminishing the influence of the power spectra amplitude. To speed up computations, the number of CPU cores was set to two.

Group-level fingerprints in the 1–40Hz frequency interval from 8 distant regions of the human brain (ROIs; Fig. 8) were found (Fig. 9). The similarity of fingerprints was assessed (Fig. 10), together with the accuracy of how well one can identify them (Fig. 11).

The proposed method allowed for discrimination between different modes of operation for a range of brain areas. Dominant and supportive group-level oscillation profiles were recognized and separated. Functional similarity between homologue areas was confirmed using hierarchical clustering analysis. Recognition of the brain areas based on their spectral fingerprints turned out to be challenging among homologue

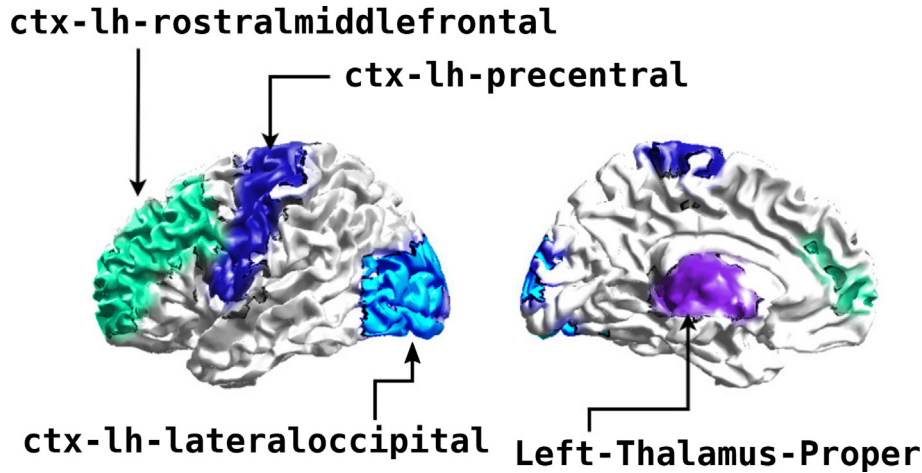


Fig. 8. Brain regions chosen from the Desikan-Killiany atlas for the purpose of the illustrative example. Here only the left counterpart is depicted, whereas right hemisphere homologues were chosen as well.

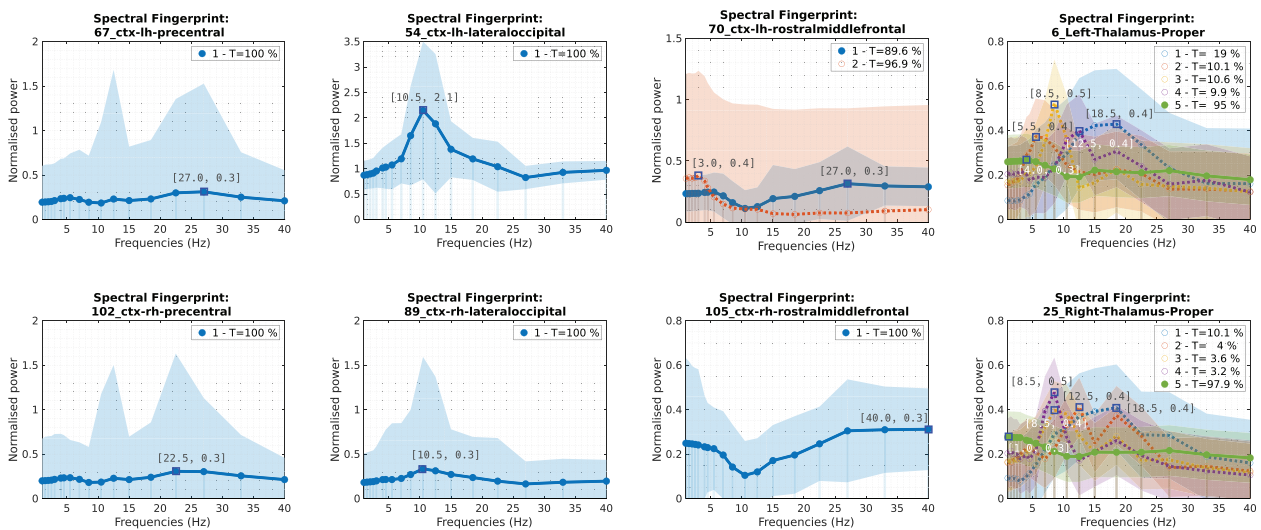


Fig. 9. Resting-state spectral fingerprints for Desikan-Killiany atlas in the 1–40 Hz frequency interval. Each column shows two homologue brain areas. Legends show the corresponding duration of each spectral mode (i.e., the percentage of trials in which each spectrum was present on average during recording) and whether the mode was present for at least five subjects (filled dot) or not (empty dot). The frequency axis was configured to be logarithmic in order to optimize the lower frequencies resolution. Y-axis depicts the power normalized in relation to the average spectrum of the whole brain. Shaded regions depict the standard deviation (1σ) of the corresponding spectral mode. For i -th of total F frequencies of interest, standard deviation was estimated as $\sqrt{\sum_{i,j} \Sigma_{i,j}}$, where $\Sigma_{i,j}$ is the i -th diagonal entry of the covariance matrix of the Gaussian Mixture Model component corresponding to the given spectral mode. Standard deviations have relatively large values due to the small number of subjects used in the illustrative example. Homologue areas have very similar fingerprints.

areas due to their functional similarity, yet remaining informative.

6. Conclusions

Spectral Fingerprinting allows for the discovery of meaningful oscillatory patterns from electrophysiological time series that can show task-induced modulations or serve as a signature of the brain’s regional activity in the particular parcellation. Our novel Toolbox for Frequency-based Fingerprinting (ToFFi) provides researchers with a modular, highly configurable tool for computing regional source-reconstructed power spectra, finding optimal prototypes common for a group of subjects via individual- and group-level clustering algorithms, together with testing their properties

using additional analytical routines. The efficiency is boosted with parallel computation support, and reproducibility is controlled with pseudo-random number generator parameters. An in-depth understanding of the underlying algorithms is facilitated by the function reference (Appendix B) and the toolbox manual (Appendix A). Presented software is compatible with various modern tools used by the neuroscientific community and allows easy adaptation of its modular structure to specific tasks.

There is high applicational potential in using ToFFi. Constructing spectral representations of regional activity, i.e., brain fingerprints, could help study cortical and subcortical activity modulation during cognitive processing in healthy and diseased brains. Compounding such knowledge and correlating fingerprint features with behavioral measurements could ultimately lead to the construction of normative databases of cognition, which in turn

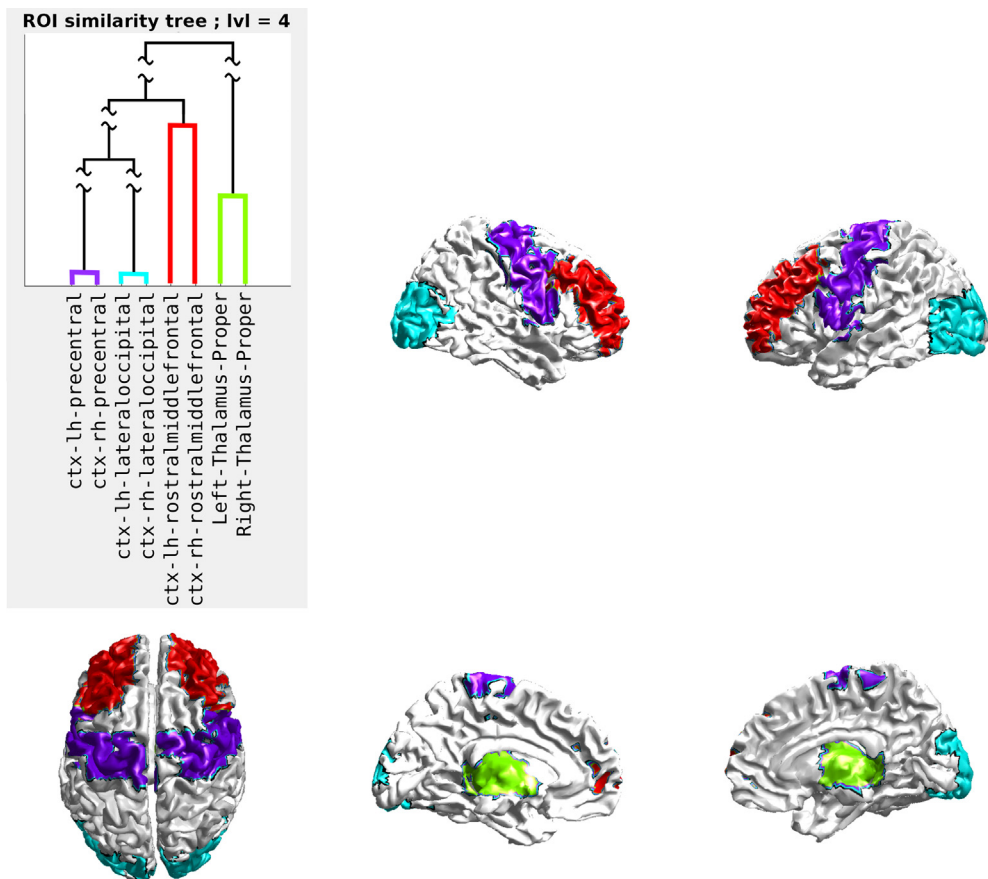


Fig. 10. Result of the hierarchical agglomerative clustering of the spectral fingerprints presented in Fig. 9. Homologue areas were automatically matched together according to the similarity of their fingerprints. The similarity tree has disproportionately long branches that were broken for clarity (waved lines).

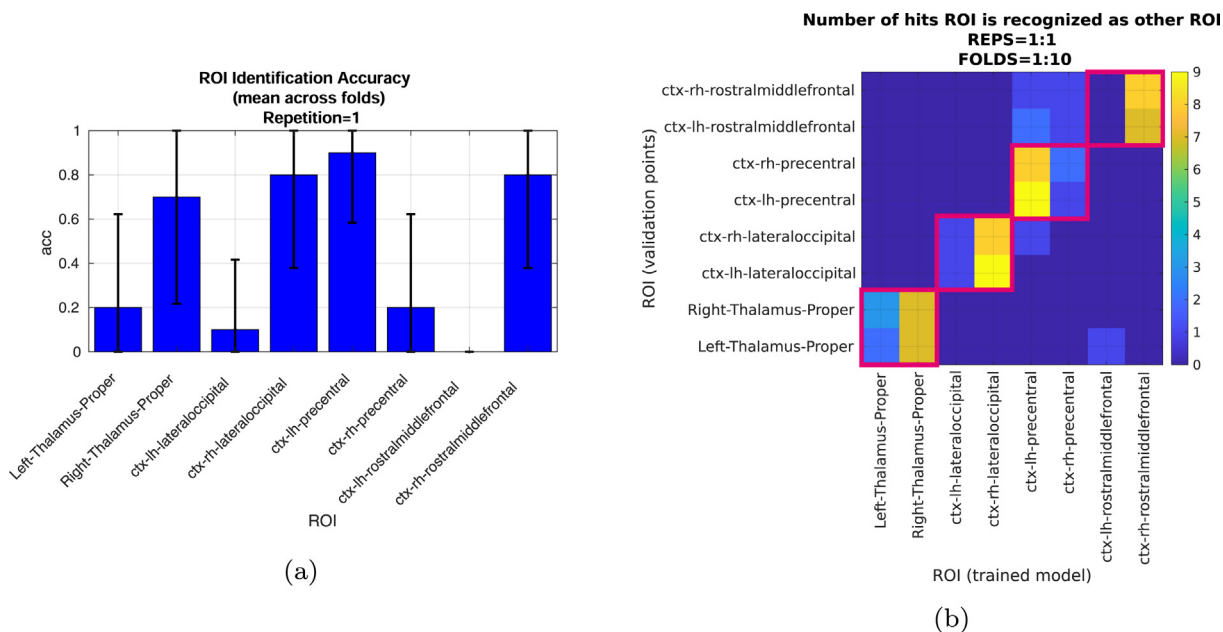


Fig. 11. Group-level identification accuracy: a) bar plot showing the average identification accuracy across cross-validation iterations (leave-one-out), b) confusion matrix showing in each row a distribution of "votes" for each ROI. Each ROI was tested ten times (model trained on nine subjects versus one validation subject). For ideal identification, this matrix would have a value of 10 for the diagonal elements and zeros elsewhere. Confusion happens mostly between homologue areas (2x2 red boxes). Left hemisphere ROIs are recognized as the right hemisphere homologue areas.

Table 2
Code metadata (mandatory)

Nr.	Code metadata description	Please fill in this column
C1	Current code version	20211013
C2	Permanent link to code/ repository used of this code version	https://github.com/micholeodon/ ToFFi_Toolbox
C3	Legal Code License	GNU Lesser General Public License v2.1
C4	Code versioning system used	Git
C5	Software code languages, tools, and services used	MATLAB, Bash
C6	Compilation requirements, operating environments & dependencies	None
C7	If available Link to developer documentation/manual	https://github.com/micholeodon/ ToFFi_Toolbox/tree/master/ ToFFi_Toolbox-20211013/docs/ ToFFi_Manual.pdf
C8	Support email for questions	michu.kom@gmail.com

be of much value to researchers and clinicians. Finally, considering biometric applications, it would be interesting to test if it is possible to identify subjects from their brain spectral fingerprints constructed with ToFFi.

CRedit authorship contribution statement

Michał K. Komorowski: Conceptualization, Investigation, Methodology, Software, Validation, Formal analysis, Data curation, Writing - original draft, Writing - review & editing, Visualization. **Krzysztof Rykaczewski:** Formal analysis, Writing - review & editing. **Tomasz Piotrowski:** Conceptualization, Writing - review & editing, Supervision. **Katarzyna Jurewicz:** Conceptualization, Formal analysis, Writing - review & editing. **Jakub Wojciechowski:** Conceptualization, Formal analysis, Writing - review & editing. **Anne Keitel:** Validation, Writing - review & editing, Resources. **Joanna Dreszer:** Conceptualization, Supervision, Methodology. **Włodzisław Duch:** Conceptualization, Writing - review & editing, Resources, Supervision, Funding acquisition, Project administration.

Data availability

Research data and code are publicly and available free of charge in repositories mentioned in the article text.

Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

Acknowledgments

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Appendix A. ToFFi toolbox manual

Link: [https://github.com/micholeodon/ToFFi_Toolbox/
tree/master/ToFFi_Toolbox-20211013/docs/ToFFi_Manual.pdf](https://github.com/micholeodon/ToFFi_Toolbox/tree/master/ToFFi_Toolbox-20211013/docs/ToFFi_Manual.pdf)

Appendix B. Functions reference

Functions reference documents most important M-File Functions of the ToFFi Toolbox.

It can be accessed **after** downloading/cloning the ToFFi Toolbox repository (https://github.com/micholeodon/ToFFi_Toolbox).

Functions reference can be found here:

`TOFFi_Toolbox-YYYYMMDD/docs/FUNCTIONS_REFERENCE.html`, where YYYYMMDD stands for the toolbox revision number.

Appendix C. Required Metadata

C.1. Current executable software version

Table 1

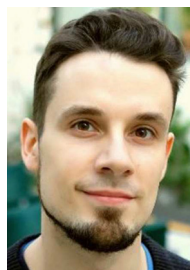
Appendix D. Current code version

Table 2

References

- [1] M. Bola, B.A. Sabel, Dynamic reorganization of brain functional networks during cognition, *NeuroImage* 114 (2015) 398–413, <https://doi.org/10.1016/j.neuroimage.2015.03.057>.
- [2] F.M. Krienen, B.T.T. Yeo, R.L. Buckner, Reconfigurable task-dependent functional coupling modes cluster around a core functional architecture, *Philos. Trans. R. Soc. B: Biol. Sci.* 369 (1653) (2014) 20130526, <https://doi.org/10.1098/rstb.2013.0526>.
- [3] R. Ciric, J.S. Nomi, L.Q. Uddin, A.B. Satpute, Contextual connectivity: A framework for understanding the intrinsic dynamic architecture of large-scale functional brain networks, *Sci. Rep.* 7 (1) (2017) 6537, <https://doi.org/10.1038/s41598-017-06866-w>.
- [4] J.N. Keynan, Y. Meir-Hasson, G. Gilam, A. Cohen, G. Jackont, S. Kinreich, L. Ikar, A. Or-Borichev, A. Etkin, A. Gyurak, I. Klovatch, N. Intrator, T. Hendler, Limbic Activity Modulation Guided by Functional Magnetic Resonance Imaging-Inspired Electroencephalography Improves Implicit Emotion Regulation, *Biol. Psychiatry* 80 (6) (2016) 490–496, <https://doi.org/10.1016/j.biopsych.2015.12.024>.
- [5] M. Siegel, T.H. Donner, A.K. Engel, Spectral fingerprints of large-scale neuronal interactions, *Nat. Rev. Neurosci.* 13 (2) (2012) 121–134, <https://doi.org/10.1038/nrn3137>.
- [6] M.S. Mellem, S. Wohltjen, S.J. Gotts, A.S. Ghuman, A. Martin, Intrinsic frequency biases and profiles across human cortex, *J. Neurophysiol.* 118 (5) (2017) 2853–2864, <https://doi.org/10.1152/jn.00061.2017>.
- [7] A. Keitel, J. Gross, Individual human brain areas can be identified from their characteristic spectral activation fingerprints, *PLoS Biol* 14 (6) (2016), <https://doi.org/10.1371/journal.pbio.1002498>.
- [8] K. Mahjoory, J.-M. Schoffelen, A. Keitel, J. Gross, The frequency gradient of human resting-state brain oscillations follows cortical hierarchies, *eLife* 9 (2020), <https://doi.org/10.7554/eLife.53715>.
- [9] J. Samogin, Q. Liu, M. Marino, N. Wenderoth, D. Mantini, Shared and connection-specific intrinsic interactions in the default mode network, *NeuroImage* 200 (2019) 474–481, <https://doi.org/10.1016/j.neuroimage.2019.07.007>.
- [10] M. Marino, Q. Liu, J. Samogin, F. Tecchio, C. Cottone, D. Mantini, C. Porcaro, Neuronal dynamics enable the functional differentiation of resting state networks in the human brain, *Hum. Brain Mapp.* 40 (5) (2019) 1445–1457, <https://doi.org/10.1002/hbm.24458>.
- [11] C.D. Hacker, A.Z. Snyder, M. Pahwa, M. Corbetta, E.C. Leuthardt, Frequency-specific electrophysiologic correlates of resting state fMRI networks, *NeuroImage* 149 (2017) 446–457, <https://doi.org/10.1016/j.neuroimage.2017.01.054>.
- [12] M. Rosanova, A. Casali, V. Bellina, F. Resta, M. Mariotti, M. Massimini, Natural Frequencies of Human Corticothalamic Circuits, *J. Neurosci.* 29 (24) (2009) 7679–7685, <https://doi.org/10.1523/JNEUROSCI.0445-09.2009>.
- [13] L.A. Farwell, E. Donchin, The Truth Will Out: Interrogative Polygraphy ("Lie Detection") With Event-Related Brain Potentials, *Psychophysiology* 28 (5) (1991) 531–547, <https://doi.org/10.1111/j.1469-8986.1991.tb01990.x>.
- [14] L.A. Farwell, Brain fingerprinting: A comprehensive tutorial review of detection of concealed information with event-related brain potentials,

- Cogn. Neurodyn. 6 (2) (2012) 115–154, <https://doi.org/10.1007/s11571-012-9192-2>.
- [15] M.U. Afzali, A.P. Seren-Grace, R.W. Palmer, E. Neumann, S. Makarious, D. Wilson, R.D. Jones, Detection of concealed knowledge via the ERP-based technique Brain Fingerprinting: Real-life and real-crime incidents, *Psychophysiology* n/a (n/a) (2022) e14110. doi:10.1111/psyp.14110.
- [16] O. Miranda-Dominguez, B.D. Mills, S.D. Carpenter, K.A. Grant, C.D. Kroenke, J.T. Nigg, D.A. Fair, Connectotyping: Model Based Fingerprinting of the Functional Connectome, *PLOS ONE* 9 (11) (2014), <https://doi.org/10.1371/journal.pone.0111048>.
- [17] E.S. Finn, X. Shen, D. Scheinost, M.D. Rosenberg, J. Huang, M.M. Chun, X. Papademetris, R.T. Constable, Functional connectome fingerprinting: Identifying individuals using patterns of brain connectivity, *Nat. Neurosci.* 18 (11) (2015) 1664–1671, <https://doi.org/10.1038/nn.4135>.
- [18] C. Wachinger, P. Golland, W. Kremen, B. Fischl, M. Reuter, Alzheimer's Disease Neuroimaging Initiative, BrainPrint: A discriminative characterization of brain morphology, *NeuroImage* 109 (2015) 232–248, <https://doi.org/10.1016/j.neuroimage.2015.01.032>.
- [19] K. Kumar, C. Desrosiers, K. Siddiqi, O. Colliot, M. Toews, Fiberprint: A subject fingerprint based on sparse code pooling for white matter fiber analysis, *NeuroImage* 158 (2017) 242–259, <https://doi.org/10.1016/j.neuroimage.2017.06.083>.
- [20] K. Kumar, M. Toews, L. Chauvin, O. Colliot, C. Desrosiers, Multi-modal brain fingerprinting: A manifold approximation based framework, *NeuroImage* 183 (2018) 212–226, <https://doi.org/10.1016/j.neuroimage.2018.08.006>.
- [21] L. Chauvin, K. Kumar, C. Wachinger, M. Vangel, J. de Guise, C. Desrosiers, W. Wells, M. Toews, Neuroimage signature from salient keypoints is highly specific to individuals and shared by close relatives, *NeuroImage* 204 (2020), <https://doi.org/10.1016/j.neuroimage.2019.116208>.
- [22] L. Chauvin, K. Kumar, C. Desrosiers, W. Wells, M. Toews, Efficient Pairwise Neuroimage Analysis Using the Soft Jaccard Index and 3D Keypoint Sets, *IEEE Trans. Med. Imaging* 41 (4) (2022) 836–845, <https://doi.org/10.1109/TMI.2021.3123252>.
- [23] M. DelPozo-Banos, C.M. Travieso, C.T. Weidemann, J.B. Alonso, EEG biometric identification: A thorough exploration of the time-frequency domain, *J. Neural Eng.* 12 (5) (2015), <https://doi.org/10.1088/1741-2560/12/5/056019>.
- [24] B.C. Armstrong, M.V. Ruiz-Blondet, N. Khalifian, K.J. Kurtz, Z. Jin, S. Laszlo, Brainprint: Assessing the uniqueness, collectability, and permanence of a novel method for ERP biometrics, *Neurocomputing* 166 (2015) 59–67, <https://doi.org/10.1016/j.neucom.2015.04.025>.
- [25] H. van Dijk, J.-M. Schoffelen, R. Oostenveld, O. Jensen, Prestimulus Oscillatory Activity in the Alpha Band Predicts Visual Discrimination Ability, *J. Neurosci.* 28 (8) (2008) 1816–1823, <https://doi.org/10.1523/JNEUROSCI.1853-07.2008>.
- [26] J.T. Baker, D.G. Dillon, L.M. Patrick, J.L. Roffman, R.O. Brady, D.A. Pizzagalli, D. Öngür, A.J. Holmes, Functional connectomics of affective and psychotic pathology, *Proc. Natl. Acad. Sci.* 116(18) (2019) 9050–9059. doi:10.1073/pnas.1820780116.
- [27] C. Lubinus, J. Orpella, A. Keitel, H. Gudi-Mindermann, A.K. Engel, B. Roeder, J.M. Rimele, Data-Driven Classification of Spectral Profiles Reveals Brain Region-Specific Plasticity in Blindness, *Cereb. Cortex* 31 (5) (2021) 2505–2522, <https://doi.org/10.1093/cercor/bhaa370>.
- [28] M. Congedo, R.E. John, D. De Ridder, L. Prichep, Group independent component analysis of resting state EEG in large normative samples, *Int. J. Psychophysiol.* 78 (2) (2010) 89–99, <https://doi.org/10.1016/j.ijpsycho.2010.06.003>.
- [29] A. Hillebrand, G.R. Barnes, J.L. Bosboom, H.W. Berendse, C.J. Stam, Frequency-dependent functional connectivity within resting-state networks: An atlas-based MEG beamformer solution, *NeuroImage* 59 (4) (2012) 3909–3921, <https://doi.org/10.1016/j.neuroimage.2011.11.005>.
- [30] J.F. Hipp, D.J. Hawellek, M. Corbetta, M. Siegel, A.K. Engel, Large-scale cortical correlation structure of spontaneous oscillatory activity, *Nat. Neurosci.* 15 (6) (2012) 884–890, <https://doi.org/10.1038/nn.3101>.
- [31] Y. Meir-Hasson, S. Kinreich, I. Podlipsky, T. Hendler, N. Intrator, An EEG Fingerprint of fMRI deep regional activation, *NeuroImage* 102 (2014) 128–141, <https://doi.org/10.1016/j.neuroimage.2013.11.004>.
- [32] P. Ramkumar, L. Parkkonen, A. Hyvärinen, Group-level spatial independent component analysis of Fourier envelopes of resting-state MEG data, *NeuroImage* 86 (2014) 480–491, <https://doi.org/10.1016/j.neuroimage.2013.10.032>.
- [33] J.N. Keyman, Y. Meir-Hasson, G. Gilam, A. Cohen, G. Jackont, S. Kinreich, L. Ikar, A. Or-Borichev, A. Etkin, A. Gyurak, I. Klovatch, N. Intrator, T. Hendler, Limbic Activity Modulation Guided by Functional Magnetic Resonance Imaging-Inspired Electroencephalography Improves Implicit Emotion Regulation, *Biol. Psychiatry* 80 (6) (2016) 490–496, <https://doi.org/10.1016/j.biopsych.2015.12.024>.
- [34] M.F. Glasser, T.S. Coalson, E.C. Robinson, C.D. Hacker, J. Harwell, E. Yacoub, K. Ugurbil, J. Andersson, C.F. Beckmann, M. Jenkinson, S.M. Smith, D.C. Van Essen, A multi-modal parcellation of human cerebral cortex, *Nature* 536 (7615) (2016) 171–178, <https://doi.org/10.1038/nature18933>.
- [35] T.H. Donner, M. Siegel, A framework for local cortical oscillation patterns, *Trends Cognit. Sci.* 15 (5) (2011) 191–199, <https://doi.org/10.1016/j.tics.2011.03.007>.
- [36] W. Singer, Cortical dynamics revisited, *Trends Cognit. Sci.* 17 (12) (2013) 616–626, <https://doi.org/10.1016/j.tics.2013.09.006>.
- [37] F. Ferrarelli, S. Sarasso, Y. Guller, B.A. Riedner, M.J. Peterson, M. Bellesi, M. Massimini, B.R. Postle, G. Tononi, Reduced natural oscillatory frequency of frontal thalamocortical circuits in schizophrenia, *Arch. Gen. Psychiatry* 69 (8) (2012) 766–774, <https://doi.org/10.1001/archgenpsychiatry.2012.147>.
- [38] R. Oostenveld, P. Fries, E. Maris, J.-M. Schoffelen, FieldTrip: Open Source Software for Advanced Analysis of MEG, EEG, and Invasive Electrophysiological Data, *Comput. Intell. Neurosci.* 2011 (2010), <https://doi.org/10.1155/2011/156869>.
- [39] A. Delorme, S. Makeig, EEGLAB: an open source toolbox for analysis of single-trial EEG dynamics including independent component analysis, *J. Neurosci. Methods* 134 (1) (2004) 9–21, <https://doi.org/10.1016/j.jneumeth.2003.10.009>.
- [40] K. Rykaczewski, J. Nikadon, W. Duch, T. Piotrowski, supFunSim: Spatial Filtering Toolbox for EEG, *Neuroinformatics* 19 (1) (2021) 107–125, <https://doi.org/10.1007/s12021-020-09464-w>.
- [41] P. Sanz Leon, S.A. Knock, M.M. Woodman, L. Domide, J. Mersmann, A.R. McIntosh, V. Jirsa, The Virtual Brain: a simulator of primate brain network dynamics, *Front. Neuroinform.* 7. doi:10.3389/fninf.2013.00010.
- [42] B. Van Veen, W. Van Drongelen, M. Yuchtman, A. Suzuki, Localization of brain electrical activity via linearly constrained minimum variance spatial filtering, *IEEE Trans. Biomed. Eng.* 44 (9) (1997) 867–880, <https://doi.org/10.1109/10.623056>.
- [43] K. Sekihara, S.S. Nagarajan, Adaptive Spatial Filters for Electromagnetic Brain Imaging, *Series in Biomedical Engineering*, Springer-Verlag, Berlin Heidelberg (2008), <https://doi.org/10.1007/978-3-540-79370-0>.
- [44] N. Tzourio-Mazoyer, B. Landeau, D. Papathanassiou, F. Crivello, O. Etard, N. Delcroix, B. Mazoyer, M. Joliot, Automated anatomical labeling of activations in SPM using a macroscopic anatomical parcellation of the MNI MRI single-subject brain, *NeuroImage* 15 (1) (2002) 273–289, <https://doi.org/10.1006/nimg.2001.0978>.
- [45] R.S. Desikan, F. Ségonne, B. Fischl, B.T. Quinn, B.C. Dickerson, D. Blacker, R.L. Buckner, A.M. Dale, R.P. Maguire, B.T. Hyman, M.S. Albert, R.J. Killiany, An automated labeling system for subdividing the human cerebral cortex on MRI scans into gyral based regions of interest, *NeuroImage* 31 (3) (2006) 968–980, <https://doi.org/10.1016/j.neuroimage.2006.01.021>.
- [46] A. Schaefer, R. Kong, E.M. Gordon, T.O. Laumann, X.-N. Zuo, A.J. Holmes, S.B. Eickhoff, B.T.T. Yeo, Local-Global Parcellation of the Human Cerebral Cortex from Intrinsic Functional Connectivity MRI, *Cerebral Cortex* (New York, N.Y.: 1991) 28 (9) (2018) 3095–3114. doi:10.1093/cercor/bhx179.
- [47] D.C. Van Essen, S.M. Smith, D.M. Barch, T.E. Behrens, E. Yacoub, K. Ugurbil, The WU-Minn Human Connectome Project: An Overview, *NeuroImage* 80 (2013) 62–79, <https://doi.org/10.1016/j.neuroimage.2013.05.041>.



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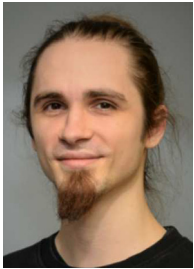
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