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# Validity and reliability of seismocardiography for the estimation of cardiorespiratory fitness



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**BACKGROUND** Low cardiorespiratory fitness (ie, peak oxygen consumption  $[\dot{V}0_2peak]$ ) is associated with cardiovascular disease and all-cause mortality and is recognized as an important clinical tool in the assessment of patients. Cardiopulmonary exercise test (CPET) is the gold standard procedure for determination of  $\dot{V}0_2peak$  but has methodological challenges as it is time-consuming and requires specialized equipment and trained professionals. Seismofit is a chest-mounted medical device for estimating  $\dot{V}0_2peak$  at rest using seismocardiography.

**OBJECTIVE** The purpose of this study was to investigate the validity and reliability of Seismofit  $\dot{V}0_2$  peak estimation in a healthy population.

**METHODS** On 3 separate days, 20 participants (10 women) underwent estimations of  $\dot{V}0_2$ peak with Seismofit ( $\times$ 2) and Polar Fitness Test (PFT) in randomized order and performed a graded CPET on a cycle ergometer with continuous pulmonary gas exchange measurements.

**RESULTS** Seismofit  $\dot{V}0_2$ peak showed a significant bias of -3.1  $\pm$  2.4 mL·min<sup>-1</sup>·kq<sup>-1</sup> (mean  $\pm$  95% confidence interval) and 95%

limits of agreement (LoA) of  $\pm 10.8~\text{mL}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$  compared to CPET. The mean absolute percentage error (MAPE) was 12.0%. Seismofit  $\dot{V}0_2$ peak had a coefficient of variation of 4.5%  $\pm$  1.3% and an intraclass correlation coefficient of 0.95 between test days and a bias of 0.0  $\pm$  0.4  $\text{mL}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$  with 95% LoA of  $\pm 1.6~\text{mL}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$  in test–retest. In addition, Seismofit showed a 2.4  $\text{mL}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$  smaller difference in 95% LoA than PFT compared to CPET.

**CONCLUSION** The Seismofit is highly reliable in its estimation of  $\dot{V}0_2$ peak. However, based on the measurement error and MAPE >10%, the Seismofit  $\dot{V}0_2$ peak estimation model needs further improvement to be considered for use in clinical settings.

**KEYWORDS** Seismocardiography;  $VO_2$ max estimation; Nonexercise  $VO_2$ peak equation; Cardiorespiratory fitness test; Method agreement

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#### Introduction

Cardiorespiratory fitness is a powerful independent predictor of cardiovascular disease (CVD) and all-cause mortality. <sup>1-4</sup> Measurement of peak oxygen consumption (VO<sub>2</sub>peak) during a graded cardiopulmonary exercise test (CPET) is considered the gold standard method for the determination of cardiorespiratory fitness. <sup>1,5</sup> Routine assessment of VO<sub>2</sub>peak in the clinical setting is recommended by the

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American Heart Association (AHA)<sup>1</sup> because it significantly improves CVD risk classification compared to traditional CVD risk models.<sup>6,7</sup> Furthermore, even a small increment in VO2peak is found to be associated with reduced mortality risk<sup>8,9</sup> and reduced risk of future CVD readmission in cardiac patients. 10 The AHA recommendation has not yet been successfully adopted, as it might not be possible or feasible to perform exercise testing during most patient encounters. 11 Nonexercise estimation of VO2peak has been proposed as a pragmatic alternative to CPET. 1,11-14 Due to recent advantages in heart rate monitoring technology that allow estimation of VO<sub>2</sub>peak to be performed in the resting condition, Polar Electro Oy (Kempele, Finland) created the Polar Fitness Test (PFT), which uses age, body weight, height, and self-reported weekly training hours together with resting heart rate and heart rate variability to estimate

#### **KEY FINDINGS**

- The reliability of the Seismofit peak oxygen consumption  $(\dot{V}0_2\text{peak})$  estimation was high both within and between test days.
- ullet The Seismofit underestimated  $\dot{V}0_2$  peak compared to the gold standard measurement and the mean absolute percentage error was above the predefined level of 10% for clinical relevance.
- The reliability indicates that the Seismofit is dependable in recording and processing the seismocardiography signal. Thus, it is expected that Seismofit VO<sub>2</sub>peak estimation will improve when more data are available for training the algorithm.

 $\dot{V}O_2$  peak. However, the validity of the PFT is still considered inadequate for application in clinical health care and in sports. 15-17 Seismocardiography (SCG) is a technique for noninvasive evaluation of cardiac activity through the measurement of precordial vibrations accelerometer. 18-20 The complexity of SCG signals has previously been a challenge; however, the new advantages of low-cost lightweight sensors, signal processing, feature extraction, and machine learning methods have made the SCG methodology relevant for clinical application.<sup>20</sup> It is widely accepted that maximal cardiac output (ie, maximal heart rate and stroke volume) is the primary factor limiting VO<sub>2</sub>peak in the healthy population, <sup>21</sup> and this is highly dependent on diastolic function. <sup>22</sup> A faster relaxation and increase in diastolic filling would increase cardiac output and thus VO<sub>2</sub>peak (ie, the Frank-Starling law). Fiducial points in the resting SCG signal have previously been shown to correlate with characteristic events in the cardiac cycle<sup>23</sup> and provide information on ventricular performance.<sup>24</sup> In addition, a high correlation between the diastolic SCG peak-to-peak value (fiducial point C<sub>d</sub> to D<sub>d</sub>) and the diastolic relaxation parameter e' measured by echocardiography in the resting condition has recently been established.<sup>25</sup> Functionally, a faster relaxation would lead to a more rapid drop in left ventricular pressure, thereby creating a greater pressure difference between the left ventricle and ascending aorta, which would result in a larger amplitude of the C<sub>d</sub> to D<sub>d</sub> fiducial point.<sup>26</sup> A VO<sub>2</sub>peak estimation model using both diastolic and systolic SCG information at rest has been proposed<sup>26</sup> and validated against CPET.<sup>27,28</sup> This led to the development of a new wireless sensor device containing an accelerometer with a compatible smartphone app and a cloud-based solution for automated SCG signal processing (Seismofit system).<sup>29</sup> The Seismofit is an interesting novel solution and potentially is a clinically applicable alternative to the standard CPET. However, thorough assessment of the validity and reliability of the Seismofit estimation of VO<sub>2</sub>peak compared with the CPET is needed to evaluate the applicability of the method. This study aimed to examine

the validity and reliability of the Seismofit  $\dot{V}O_2$ peak estimation compared with CPET in a healthy population sample. It was hypothesized that the Seismofit would prove valid and reliable for estimation of  $\dot{V}O_2$ peak, with a mean absolute percentage error (MAPE)  $\leq$ 10% between methods and a withinmethod coefficient of variation (CoV)  $\leq$ 5%.

#### Methods

#### Study outline and objectives

Three identical test days separated by at least 48 hours and within 14 days were conducted to assess the validity and reliability of the Seismofit VO2peak estimation. On each test day, VO2peak was estimated twice with Seismofit (Seismofit 1 and 2) and once with PFT before being measured directly with the gold standard CPET using indirect calorimetry. CPET was used as a reference method to assess the agreement of Seismofit and PFT and to compare the reliability against the different estimation methods. The repeated Seismofit measurement within each test day was used to assess repeatability. The present study only compares estimated and measured VO<sub>2</sub>peak values performed in a clinical setting and is not addressing the algorithms behind the estimation models. Testing was conducted between June 2020 and November 2020. The study conformed to the Helsinki Declaration and was approved by the Science Ethical Committee of the Greater Region of Copenhagen, Denmark (H-19081375). The study was registered as ClinicalTrials.gov Identifier NCT05356871.

#### Study population

Twenty healthy participants were recruited (10 women, 10 men). A priori recruitment strategy including 4 trained and 4 untrained between the ages of 18 to 39 years, and 6 trained and 6 untrained between the ages of 40 to 75 years with equal distribution between sexes was completed. A detailed description of the recruitment strategy is provided in the Supplementary Materials (Supplemental Table 1). Inclusion criteria were healthy adults between the ages of 18 and 75 years. Exclusion criteria were a history of previous or current CVD, pregnancy, and/or conditions that prevent maximal exercise testing. Before volunteering and signing a written consent form, the participants received oral and written information about the study and its possible risks.

#### Experimental design

Measurements of anthropometrics and blood pressure together with collection of a resting blood sample were obtained on each test day, and body composition was determined on the first test day (Table 1). A detailed description of the measurements, experimental procedures, and equipment used is given in the Supplemental Material.

#### Estimation of $\dot{V}$ 0<sub>2</sub>peak in resting condition

The Seismofit system was used for recording of the SCG signal and estimation of  $\dot{V}O_2$ peak at supine rest. <sup>29</sup> The Seismofit system consists of a small medical device containing a

 Table 1
 Measured and estimated values from three separate test days

|  | Day 1              | Day 2                | Day 3                | Within-<br>subject<br>SD | Within-<br>subject<br>CoV% | ICC  | P-<br>value |
|--|--------------------|----------------------|----------------------|--------------------------|----------------------------|------|-------------|
| Measurements   |                    |                      |                      |                          |                            |      |             |
| Age (yrs.)   | $47 \pm 7$         | -                    | -                    | -                        | -                          | -    | -           |
| Height (cm)  | $176 \pm 4$        | -                    | -                    | -                        | -                          | -    | -           |
| Weight (kg)  | $73.7 \pm 5.1$     | $73.7 \pm 5.1$       | $73.8 \pm 5.4$       | 0.5                      | $0.6 \pm 0.1$              | 1.00 | 0.837       |
| Body fat, (%)  | $26.1 \pm 3.3$     | -                    | -                    | -                        | -                          | -    | -           |
| Systolic BP (mmHg)   | $132 \pm 9$        | $128 \pm 7$          | $128 \pm 8$          | 5                        | $3 \pm 1$                  | 0.91 | 0.063       |
| Diastolic BP (mmHg)  | $80 \pm 5$         | 77 ± 5*              | 76 ± 4*              | 4                        | 5 ± 1                      | 0.85 | 0.009       |
| HRrest (beats min-1)   | 55 ± 4             | 54 ± 4               | 54 ± 4               | 3                        | 5 ± 2                      | 0.85 | 0.280       |
| Haemoglobin (mmol/L)   | $9.2 \pm 0.4^{a}$  | $8.9 \pm 0.4^{b} *$  | $8.9 \pm 0.4^{b} *$  | 0.2                      | $2.3 \pm 0.7$              | 0.94 | 0.031       |
| Haematocrit (%)  | $45.5 \pm 2.0^{a}$ | $44.0 \pm 2.0^{b} *$ | $44.2 \pm 2.1^{b} *$ | 1.0                      | $2.2 \pm 0.6$              | 0.95 | 0.028       |
| Non-exercise V O <sub>2</sub> peak estimation                |                    |                      |                      |                          |                            |      |             |
| Seismofit 1 (ml·min <sup>-1</sup> ·kg <sup>-1</sup> )        | $36.6 \pm 3.4$     | $36.6 \pm 3.1$       | $36.6 \pm 3.4$       | 1.7                      | $4.5 \pm 1.3$              | 0.95 | 0.907       |
| Seismofit 2 (ml·min <sup>-1</sup> ·kg <sup>-1</sup> )        | $36.6 \pm 3.3$     | $36.7 \pm 3.1$       | $36.5 \pm 3.5$       | 1.5                      | $3.8 \pm 1.2$              | 0.96 | 0.872       |
| Polar Fitness Test (ml·min <sup>-1</sup> ·kg <sup>-1</sup> ) | $43.5 \pm 4.8$     | $44.9 \pm 4.8$       | $43.9 \pm 4.6$       | 1.8                      | $3.0 \pm 1.4$              | 0.97 | 0.168       |
| Cardiopulmonary exercise test                                |                    |                      |                      |                          |                            |      |             |
| $\dot{V}0_2$ peak (ml·min <sup>-1</sup> ·kg <sup>-1</sup> )  | $39.6 \pm 2.7$     | $39.7 \pm 3.1$       | $39.2 \pm 3.2^{a}$   | 1.5                      | $3.4 \pm 0.8$              | 0.95 | 0.907       |
| $\dot{V}0_2$ peak (ml·min <sup>-1</sup> )                    | $2916 \pm 293$     | $2930 \pm 315$       | $2837 \pm 289^{a}$   | 116                      | $3 \pm 1$                  | 0.97 | 0.808       |
| V <sub>E</sub> peak (L∙min <sup>-1</sup> )                   | $124 \pm 14$       | $127\pm15$           | $124 \pm 14^{a}$     | 8                        | 5 ± 2                      | 0.94 | 0.246       |
| HRpeak (beats · min <sup>-1</sup> )                          | $173 \pm 7$        | $172 \pm 6$          | $172 \pm 7^{a}$      | 3                        | $2 \pm 0$                  | 0.96 | 0.150       |
| Watt peak (W)  | $251\pm28$         | $252\pm30$           | $242 \pm 29^{a}$     | 8                        | 2 ± 1                      | 0.99 | 0.896       |

Data are presented as mean  $\pm$  95% CI. n=20.

3-axis digital output accelerometer, a smartphone app, and a cloud solution for signal processing. The SCG recording was performed with the Seismofit device mounted on the sternum with double adhesive tape 2 cm proximal to the xiphoid process (Supplemental Figure 1). Before estimation, the age, height, weight, and sex of the participant were entered into the app. VO<sub>2</sub>peak estimation lasted approximately 5 minutes, which included SCG recording, data transfer to the app, and signal processing. Subsequently, the result of the VO<sub>2</sub>peak estimation was shown in the app. The newest version, at the time of the study, of the VO<sub>2</sub>peak estimation model was used (SCG Version 4.3), which has previously been described.<sup>27</sup> The VO<sub>2</sub>peak estimation model is reproduced in Equation (1):

#### VO2 peak estimation

$$= (-15.108) + (-0.122 \cdot S2 FrequencySpec) \\ + (0.371 \cdot S2 Morphology) \\ + (0.001 \cdot RR) + (0.247 \cdot S1 FrequencySpec) \\ + (0.701 \cdot FRIENDS study prediction model) \\ + (143.4 \cdot amp\_Dd) + (-159.45 \cdot amp\_Ks) \\ + (-0.042 \cdot SYSRV\_STD) \\ + (-87.583 \cdot amp\_Ls) + (42.993 \cdot amp\_Fs) \\ (1)$$

S2FrequencySpec is analysis of the frequency spectrum of the average SCG diastolic complex quantified using principal component analysis. S2Morphology is the morphology of the average SCG diastolic complex quantified using principal component analysis. RR is the average duration of a heartbeat in milliseconds. S1FrequencySpec is a frequency measure of the average SCG systolic complex quantified using principal component analysis of the frequency spectrum of the systolic complex. The FRIENDS study prediction model is an algorithm based on sex, age, and body weight for prediction of VO<sub>2</sub>peak. 12 SYSRV\_STD is the variation in respiratory rate estimated from heart rate variability. Amp Dd, Amp\_Ks, Amp\_Ls, and Amp\_Fs are the amplitude of Dd, Ks, Ls, and Fs fiducial points, respectively (Figure 1). The definition of the fiducial points has previously been reported.<sup>23</sup> Visualization of the filtered SCG signals from 3 different test days of 1 participant is shown in Figure 1.

The patented "Polar Fitness Test" was performed at supine rest using a chest-strapped heart rate sensor (Polar H10) connected with a Polar Vantage M watch. The PFT uses demographic data (age, weight, height, sex, and training background) together with a recording of heart rate and heart rate variability. The estimation lasted approximately 5 minutes after entry of the participant's demographic data in the watch settings. The categories of training background were 0–1, 1–3, 3–5, 5–8, 8–12, and 12+ hours per week.

 $<sup>^{</sup>a}$ n=18.

 $<sup>^{\</sup>rm b}$ n=17  $^{\rm v}$ O $_2$ , oxygen consumption;  $^{\rm v}$ E, minute ventilation; HR, heart rate; Seismofit,  $^{\rm v}$ O $_2$ peak estimation model using seismocardiography version 4.3; Polar Fitness Test,  $^{\rm v}$ O $_2$ peak estimation using the Polar Fitness Test. SD; standard deviation. CoV; coefficient of variation. ICC; interclass correlation coefficient. The Watt peak is calculated using the last completed Watt stage  $^{\rm v}$  (Seconds  $^{\rm v}$ 60 seconds  $^{\rm v}$  watt increments in the representative protocol). The p-value represent the fixed effect; test day from a mixed-effect model fitted using Restricted Maximum Likelihood (REML) for assessment of systematically differences.  $^{\rm v}$ 4denotes significant different from day 1 (p<0.05).

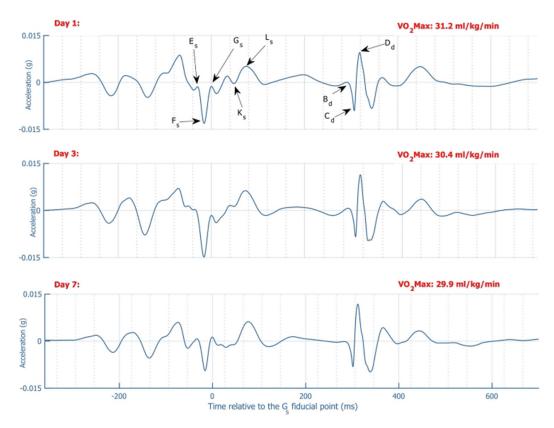


Figure 1 Filtered seismocardiography (SCG) signals from a participant on 3 separate test days together with SeismoFit peak oxygen consumption ( $\dot{V}O_2$ peak) estimation. Arrows indicate the different fiducial points used in the SeismoFit  $\dot{V}O_2$ peak estimation model with annotation of fiducial points following what is previously used in a normal SCG signal.  $B_d$  = aortic valve closure;  $C_d$  = aortic valve closure minimum point;  $D_d$  = aortic valve closure maximum point;  $E_s$  = mitral valve closure;  $F_s$  = aortic valve opening minimum point;  $G_s$  = aortic valve opening maximum point;  $G_s$  = systolic outflow minimum point;  $G_s$  = systolic outflow maximum point.

#### Determination of $\dot{V}$ 0<sub>2</sub>peak with CPET

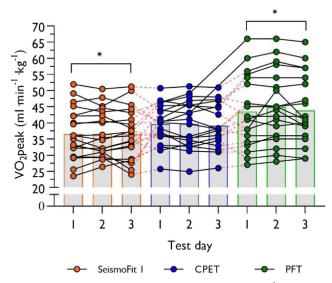
Graded CPET until voluntary exhaustion was performed on a cycle ergometer to verify whether the Seismofit VO2peak estimation could accurately determine VO<sub>2</sub>peak in healthy adults. The warm-up and initial test workload of the CPET protocol differed between sexes and training status and increased by 20 and 25 W every minute for women and men, respectively (Supplemental Table 2). The different protocols were applied to achieve a test duration of 8 to 12 minutes.<sup>31</sup> Pulmonary gas exchange was continuously obtained breath by breath during the CPET (Quark CPET, Cosmed, Rome, Italy) and sampled into 10-second intervals by an automatic online system (PFT Suite, Cosmed). Heart rate was continuously measured with a chest-strapped sensor (H10, Polar, Finland). Directly after test termination, the participants rated the perceived exhaustion on the Borg 6-20 scale.<sup>32</sup> VO<sub>2</sub>peak was calculated as the highest value measured over consecutive 30 seconds. The primary criterion for achieving VO<sub>2</sub>peak was a plateau in VO<sub>2</sub>, defined as  $<2.1 \text{ mL} \cdot \text{min}^{-1} \cdot \text{kg}^{-1}$  increment in  $\dot{V}O_2$  with increasing workload.<sup>33</sup> The secondary criteria were respiratory exchange ratio >1.10, maximal heart rate within 5 bpm of the highest measured value on the 3 test days, and  $\geq$ 18 on the Borg 6–20 scale.  $^{34,35}$   $\dot{V}O_2$ peak was accepted if the primary criterion or 2 of 3 of the secondary criteria were met. CPET data from the third test of 2 participants were excluded due to a calibration error. Data and the premises for exclusion are given in Supplemental Figure 2. A detailed description of the equipment calibration and evaluation of the  $\dot{V}O_2$ peak plateau is presented in the Supplemental Material.

#### Statistical analysis

All data were treated as normally distributed. Data are given as mean  $\pm$  95% confidence interval (CI). Agreement and prediction error of Seismofit 1 and PFT compared with CPET was determined by the following statistical analyses: Bland-Altman plot with 95% limits of agreement (BAplot), standard error of estimate (SEE), MAPE, and CoV. Pearson correlation coefficient r was used to evaluate the relation between Seismofit 1 and CPET, and between PFT and CPET.

Bland-Altman plots show the difference between the intra-method means plotted on the y-axis and the CPET mean plotted on the x-axis when CPET is the reference method.<sup>36</sup> Otherwise, the average of the 2 intra-method means is plotted on the x-axis.<sup>37</sup>

SEE was calculated using  $SEE = \sqrt{\sum \frac{(Y - Y')^2}{n-2}}$ , with Y representing CPET  $\dot{V}O_2$ peak and Y' representing Seismofit or



**Figure 2** Individual values of peak oxygen consumption ( $\dot{V}O_2$ peak) on the 3 different test days were estimated using the seismocardiography model (Seismofit) and the Polar Fitness Test (PFT) and directly measured during a graded cardiopulmonary exercise test with pulmonary gas exchange measurements (CPET). Mixed-effect model was applied, with the method and test day as fixed effects. Seismofit vs CPET: method (p=.022), test day (P=.907), interaction of method and test day (P=.907), interaction of method and test day (P=.135). \*Significantly different from CPET (P<.05).

PFT  $\dot{\text{VO}}_2\text{peak}$  values. Interpretation of SEE was very good <4.0 mL·min<sup>-1</sup>·kg<sup>-1</sup>; good 4.0–6.0 mL·min<sup>-1</sup>·kg<sup>-1</sup>; fair 6.0–8.0 mL·min<sup>-1</sup>·kg<sup>-1</sup>; poor 8.0–10.0 mL·min<sup>-1</sup>·kg<sup>-1</sup>; and very poor >10.0 mL·min<sup>-1</sup>·kg<sup>-1</sup>. The interpretation was based on previous studies using nonexercise estimations models. <sup>12,13,38</sup> MAPE  $\leq$ 10% was used as a criterion level for clinical relevance. Interpretation of Pearson r was very high >0.90; high 0.70–0.90; moderate 0.50–0.70; low 0.30–0.50; and little, if any, 0.00–0.30. <sup>39</sup>

The reliability of the test methods was assessed by the interclass correlation coefficient (ICC), within-subject SD, and CoV. Interpretation of ICC was poor <0.50; moderate 0.50-0.75; good 0.75-0.90; and excellent >0.90. within-subject SD was calculated by taking the square root of the within-subject variance. In addition, a mixedeffect model was applied to assess systematic differences between the test methods and test days for Seismofit 1 and CPET, and for PFT and CPET, respectively. Test-retest validity of Seismofit 1 and Seismofit 2 was assessed with the following analyses: BA-plot, Pearson's r and a mixedeffect model. The mixed model uses a compound symmetry covariance matrix, and is fitted using restricted maximum likelihood. This method gives the same P value and multiple comparison tests as repeated measures analysis of variance in the absence of missing values. In the presence of missing values (missing completely at random), the results can be interpreted as repeated measures analysis of variance. Statistical analyses were performed, and figures were constructed in GraphPad Prism 9.3.1 (GraphPad Software, Boston, MA) and Microsoft Excel (Microsoft Corporation, Redmond, WA).

#### Results CPET

After the exclusion of 2 recordings with measurement errors, excellent ICC and no statistically significant difference in measures of pre-exercise body weight or peak values of  $\dot{V}O_2$ , minute ventilation, heart rate, and workload were observed between test days for CPET (Table 1). A difference was observed for pre-exercise hematocrit and hemoglobin (Table 1). CPET displayed a low within-subject SD and CoV (Table 1). Individual values from the CPET are shown in Supplemental Figure 3.

#### Validity of $\dot{V}$ **0**<sub>2</sub>peak estimations

Seismofit 1 estimated  $\dot{V}O_2$ peak was, on average, 7% lower compared to CPET  $\dot{V}O_2$ peak (Figure 2). The agreement between methods showed a relatively large negative bias together with substantial 95% limits of agreement (LoA) (Figure 3C). A fair SEE (Figure 3A) together with a moderate CoV and MAPE above the predefined clinical limit for relevance were found between Seismofit 1 and CPET (Table 2). A high Pearson r was found between methods (Table 2).

In comparison, PFT estimated VO<sub>2</sub>peak was 11% higher than CPET VO<sub>2</sub>peak (Figure 2). The agreement between PFT and CPET showed a relatively large positive bias together with large 95% LoA (Figure 3D). A poor SEE (Figure 3B), a moderate CoV, and a MAPE well above the predefined clinical limit for relevance were found between PFT and CPET (Table 2). A high Pearson r was found between PFT and CPET.

#### Reliability of VO<sub>2</sub>peak estimations

Between test days, both Seismofit 1 and PFT demonstrated a low within-subject SD and CoV, together with an excellent ICC (Table 1).

Agreement analysis of the Seismofit test–retest revealed a nonsignificant bias of  $-0.0 \pm 0.4 \text{ mL} \cdot \text{min}^{-1} \cdot \text{kg}^{-1}$  (P = .993) with an acceptable 95% LoA (Figure 4B). A very high Pearson r of 0.99 was found between Seismofit 1 and Seismofit 2 (Figure 4A).

#### Discussion

The present study provides novel insight into the validity and reliability of a nonexercise estimation of  $\dot{V}O_2$ peak using SCG performed with a chest-mounted device—Seismofit—in a healthy population. The main finding was that even though Seismofit underestimated  $VO_2$ max significantly, Seismofit had a high correlation with the gold standard CPET and proved highly reliable in the estimation of  $\dot{V}O_2$ peak both within test days and between test days. In addition, the Seismofit displayed an overall better agreement with CPET than PFT.

### Validity of Seismofit $\dot{V}\mathbf{0}_2$ peak estimation

When clinical variables are measured, some degree of error is always present. Therefore, when comparing methods, when neither method provides an unequivocally correct

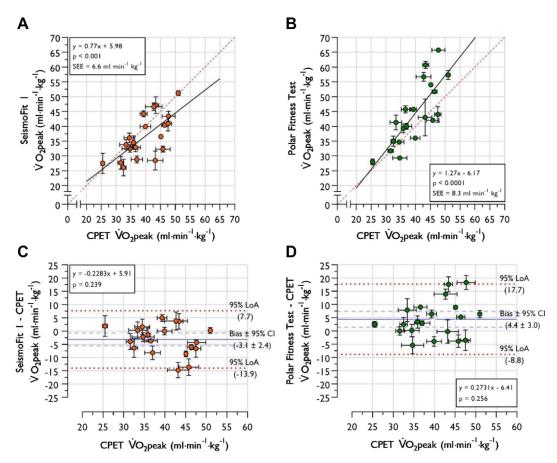


Figure 3 Data (n = 20) from of 3 separate tests for each participant (mean  $\pm$  95% confidence interval [CI]). A: Scatter plot with linear regression between  $\dot{V}O_2$  peak estimated with a nonexercise model using seismocardiography (SeismoFit 1) and directly measured during a graded cardiopulmonary exercise test with pulmonary gas exchange measurements (CPET). B: Scatter plot with linear regression between  $\dot{V}O_2$  peak estimated with the nonexercise Polar Fitness Test (PFT) and CPET. For A and B, red dotted line represents the line of identity (r = 1.0). C: Bland-Altman plot of the agreement between SeismoFit 1 and CPET. D: Bland-Altman plot of the agreement between PFT and CPET. Blue line represents the bias. Blue dotted line represents the 95% CI of the bias. Red dotted line represents the 95% LoA. Note: Two participants only have data from 2 separate tests included in the analysis. LoA = limits of agreement; SEE = standard error of estimate.

measurement, the preference is to assess the degree of agreement between methods. <sup>41</sup> Furthermore, evaluation of whether the methods agree sufficiently should be decided depending on the context in which the measurement will be used. <sup>42</sup> To the best of our knowledge, there is no accepted measurement error (systematic and random) that indicates when the agreement of a  $\dot{V}O_2$ peak estimation is acceptable

**Table 2** Accuracy between non-exercise  $\dot{V}0_2$  peak estimations and a gold standard cardiopulmonary exercise test (CPET)

|   | Pearson<br>r | Bias<br>ml·min <sup>-1</sup> ·<br>kg <sup>-1</sup> | SEE<br>ml·min <sup>-1</sup> ·<br>kg <sup>-1</sup> | MAPE<br>%    | CoV<br>%        |
|---|--------------|--|---|--------------|-----------------|
| SeismoFit 1<br>Polar<br>Fitness<br>Test | 0.70<br>0.79 | -3.1 ± 2.4*<br>4.4 ±<br>3.0*                       | 6.6<br>8.3  | 12.0<br>14.8 | 9 ± 3<br>10 ± 3 |

Data are presented as mean  $\pm$  95% CI. n=20. SeismoFit 1,  $\dot{V}$ 0<sub>2</sub>peak estimation model using seismocardiography version 4.3; Polar,  $\dot{V}$ 0<sub>2</sub>peak estimation using the Polar Fitness Test; SEE, standard error of estimate; MAPE, mean absolute percentage error. CoV; coefficient of variation.

or not. However, it has previously been suggested that the contextual validity of estimating  $\dot{V}O_2$ peak requires a measurement error within the range of 3.5 mL·kg<sup>-1</sup>·min<sup>-1</sup>, if the purpose is to assess improvement in the subject's health (ie, changes in  $\dot{V}O_2$ peak); otherwise, relevant clinical changes would be missed.<sup>42</sup> This is based on the association between a small increase in  $\dot{V}O_2$ peak (1 METS or 3.5 mL·kg<sup>-1</sup>·min<sup>-1</sup>) and a lower risk of all-cause mortality and incidence of CVD.<sup>1,4</sup> For  $\dot{V}O_2$ peak estimation models using either resting condition or exercise-based information, this still is not achieved as the estimation error at the individual level is too large.<sup>42</sup>

The present results revealed a systematic error of  $-3.1 \pm 2.4~\text{mL}\cdot\text{kg}^{-1}\cdot\text{min}^{-1}$  with a substantial total random error span of 21.6 mL·kg<sup>-1</sup>·min<sup>-1</sup>. In addition, the MAPE was above the predefined level of <10% for clinical relevance. This advocates for future efforts to improve this methodology of estimating  $\dot{V}O_2$ peak, both at the population level and in terms of evaluating individual clinically relevant changes. This is a slight contrast to a previous study applying the same SCG algorithm version, in which the model proved valid in estimating  $\dot{V}O_2$ peak at a population level, based on the

<sup>\*</sup>significantly different from CPET (p<0.05).

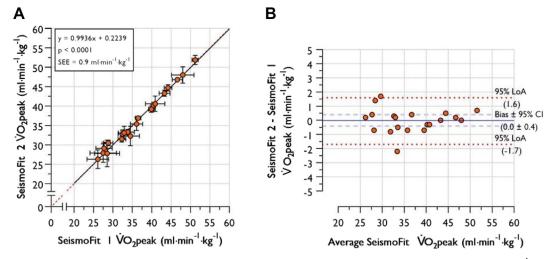


Figure 4 Data (n = 20) from 3 separate tests for each participant (mean  $\pm$  95% CI). A: Scatter plot with linear regression between 2  $\dot{V}O_2$ peak estimations performed with a nonexercise model using seismocardiography (SeismoFit 1 and SeismoFit 2). Red dotted line represents the line of identity (r = 1.0). B: Bland-Altman plot of the agreement between SeismoFit 1 and SeismoFit 2. Blue line represents the bias. Blue dotted line represents the 95% CI of the bias. Red dotted line represents the 95% LoA. Abbreviations as in Figure 3.

systematic error (n = 97; bias  $-1.0 \pm 1.2 \,\mathrm{mL \cdot kg^{-1} \cdot min^{-1}}$ ). Otherwise, the results were similar to the previous study (LoA -12.4 to  $10.4 \text{ mL} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$ ; SEE 5.9 mL·kg<sup>-1</sup>·min<sup>-1</sup>; MAPE 12.3%; CoV 8%  $\pm$  1%; Pearson r 0.73). <sup>28</sup> One reason for the discrepancy in systematic error might be related to the studied population. The data used for developing the algorithm version 4.3 consisted primarily of subjects between the ages of 18 and 45 years. In addition, a proportional error was previously observed, which indicated that the SCG 4.3 version underestimates VO<sub>2</sub>peak more the better trained the subject is.<sup>28</sup> In the present study, the 2 participants with the largest difference between Seismofit and CPET (-13.6 and -14.7 mL·kg<sup>-1</sup>·min<sup>-1</sup>) (Figure 3C) were also the participants with the overall best training status, as they both were between 70 and 72 years old with rather unusual VO2peak values of 43.2 mL·kg<sup>-1</sup>·min<sup>-1</sup> (female) and 45.8  $mL \cdot kg^{-1} \cdot min^{-1}$  (male). When participants > 70 years were removed from the analysis (n = 3), the agreement analysis showed a bias of  $-1.8 \pm 2.3 \text{ mL} \cdot \text{kg}^{-1} \cdot \text{min}^{-1} (P = .119)$ with 95% LoA ranging from −10.4 to 6.8 mL·kg<sup>-1</sup>·min<sup>-1</sup> (Supplemental Figure 4). This implies that the current Seismofit algorithm might be restricted to estimating VO<sub>2</sub>peak at a population level with an upper age limit of 70 years and that adjustments in the model are needed for expansion of the target population to the older population. In addition, a new version of the algorithm was developed right after the current study was finalized. The new 4.5 algorithm only included training data from the previous cross-sectional study with subjects ranging between 18 and 65 years of age<sup>28</sup> and no data from the current study. When the 4.5 algorithm was applied to the current data, the agreement between methods was good (Supplemental Table 4 and Supplemental Figure 5).

### Comparison of methods for $\dot{V}\textbf{0}_2$ peak estimation

A recently published meta-analysis covering 8 studies validating the PFT showed an average overestimation of  $2.2 \pm$ 

1.9 mL·kg<sup>-1</sup>·min<sup>-1</sup> (mean  $\pm$  95% CI) with LoA ranging from -13.1 to 17.4 mL·kg<sup>-1</sup>·min<sup>-1</sup> compared with CPET. 42 In addition, 3 of the 4 most recently published studies using PFT algorithms probably are most comparable to the PFT algorithm applied in this study. These studies showed bias and 95% CI between  $3.0 \pm 3.1 \text{ mL} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$ and  $4.7 \pm 3.4 \text{ mL} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}, ^{15-17}$  whereas the fourth study found a bias of  $-0.5 \pm 2.8 \text{ mL} \cdot \text{kg}^{-1} \cdot \text{min}^{-1}$ compared with CPET. 43 Even though the PFT algorithm may have been adjusted to improve the estimate of  $\dot{V}O_2$  peak, these findings are in line with the present bias of  $4.4 \pm 3.1$  $mL \cdot kg^{-1} \cdot min^{-1}$  and thus further highlight that PFT overestimates VO<sub>2</sub>peak compared with CPET. When the validity of the Seismofit and PFT VO<sub>2</sub>peak estimations was compared, they both showed an inadequate agreement; however, the difference in LoA was smaller by 2.4 mL·kg<sup>-1</sup>·min<sup>-1</sup> and the MAPE lower by 2.8% points for the Seismofit, indicating a better agreement than PFT. The Seismofit estimation is entirely objective, in contrast to PFT where self-reported weekly hours influence the estimated VO<sub>2</sub>peak. This is a strength in the Seismofit model as people often tend to overestimate their activity level, and perhaps this is the reason for PFT overestimating VO<sub>2</sub>peak.

## Reliability of $\dot{V}\mathbf{0}_2$ peak measurement and estimation

Reliability assessment in method comparison studies is often lacking, probably due to requirements of an extended study design. However, when incorporated it provides important knowledge in the understanding of the quality of the method. Directly measured  $\dot{V}O_2$  during a graded CPET is considered the most accurate method for determination of  $\dot{V}O_2$ peak, and reproducibility typically is reported with CoV around 5%. Reliability of CPET in the present study was high, with excellent ICC and within-subject CoV of 3.4% between test days observed. Therefore, CPET was considered

acceptable as a reference method. Based on excellent ICC and within-subject CoV of 4.5% (Seismofit 1) and 3.8% (Seismofit 2), Seismofit VO<sub>2</sub>peak estimation is highly reliable between test days. Furthermore, the test–retest also proved that Seismofit repeatability was high. The consistency in within-subject VO<sub>2</sub>peak estimations is vital because it confirms that SCG signal recording, features, and fiducial point extraction and processing by the Seismofit are reliable. This indicates that the lack of accuracy probably is algorithm-dependent and not related to Seismofit SCG signal recording. SCG algorithm version 4.3 is trained using data from <150 healthy subjects within a relatively small age span, who performed a resting SCG recording and a CPET cycle ergometer test.<sup>26,27</sup>

PFT has previously been concluded to be reliable based on Pearson r = 0.91 between 2 test days. <sup>43</sup> In the present study, PFT was proved highly reliable between 3 test days, with within-subject CoV of  $3.0\% \pm 1.4\%$  and ICC of 0.97.

#### **Study limitations**

The lack of a familiarization test day for the participants to the used equipment and exercise testing is a limitation. However, it was prioritized to include a third test day instead, as few method validation studies include more than 2 test days. There were no differences in the measured  $\dot{V}O_2$ peak values between test days. The recruitment of the trained elderly participants is a limitation as they might not reflect the trained elderly population in general, but rather the very top end. Lastly, an obvious limitation is missing the 2 CPET tests due to measurement error and not including a fourth test day within a reasonable timeframe.

#### Conclusion

In the current study, Seismofit VO<sub>2</sub>peak estimation correlated to the gold standard CPET but underestimated VO<sub>2</sub>peak with a significant systematic error. Compared to PFT, Seismofit showed better agreement based on a smaller random error and MAPE. The reliability of Seismofit VO2peak estimation was high both within test days and between test days, with CoV being low and ICC excellent, indicating that the Seismofit system is dependable in recording and processing the SCG signal. Consequently, because the VO<sub>2</sub>peak estimation model is cloud-based, it is possible that Seismofit VO<sub>2</sub>peak estimation could improve and eventually be considered applicable in clinical settings when more data are available for training the algorithm. Thus, based on the present findings, the Seismofit VO<sub>2</sub>peak estimation model needs further improvement if it is to be considered for use in a clinical setting.

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#### **Disclosures**

VentriJect Aps support two-thirds of Dr Mikkel Hansen's scholarship. Dr Samuel Emil Schmidt and Dr Kasper Sørensen hold shares in VentriJect Aps. Dr Schmidt works part-time as Chief Scientific Officer and Dr Sørensen full-time as Head of Software at VentriJect Aps. There was no restriction on publication. Declaration of Generative AI and AI-assisted Technologies in the writing process: No generative AI or AI-assisted technologies have been used in the preparation of this work.

#### **Authorship**

All authors attest they meet the current ICMJE criteria for authorship.

#### **Patient Consent**

All patients provided written consent.

#### **Ethics Statement**

The study conforms to the Helsinki Declaration and was approved by the Science Ethical Committee of the Greater Region of Copenhagen, Denmark (H-19081375).

#### Data availability

All data that were used in the current study are available upon reasonable request. The estimated and measured  $\dot{V}O_2$ peak values on the 3 test days from all the participants are given in Supplemental Table 3.

#### **Appendix**

#### Supplementary data

Supplementary data associated with this article can be found in the online version at https://doi.org/10.1016/j.cvdhj.2023. 08.020.

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