

Turbulence suppression by cardiac-cycle-inspired driving of pipe flow

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Flows through pipes and channels are in practice almost always turbulent, and the multi-scale eddying motion is responsible for the major part of the encountered friction losses and pumping costs¹. Conversely, for pulsatile flows, in particular for aortic blood flow, turbulence levels remain surprisingly low despite relatively large peak velocities. Indeed, in this latter case, high turbulence levels are intolerable as they would damage the shear sensitive endothelial cell layer²⁻⁵. We here show that turbulence in ordinary pipe flow is diminished if the flow is driven in a pulsatile mode that incorporates all the key features of the cardiac waveform. At Reynolds numbers comparable to aortic blood flow, turbulence is largely inhibited, whereas, at much higher speeds, the turbulent drag is reduced by more than 25%. This specific operation mode is more efficient when compared to steady driving, which is the status quo for virtually all fluid transport processes ranging from heating circuits to water, gas and oil pipelines.

Turbulent flows are ubiquitous in nature and applications and are associated with large fric-

21 tion levels and high pumping costs when compared to laminar conditions. Available estimates
22 show that around 10% of global electric power is consumed for pumping fluids ⁶. In this context,
23 turbulence is not only encountered at large scales, such as in oil or gas pipelines, but equally domi-
24 nates flows in domestic settings (e.g. in heating pipes or the flow from a faucet). Even aortic blood
25 flow in humans and large mammals periodically exceeds transition thresholds. Compared to a tran-
26 sition Reynolds number of $Re_c \approx 2\,040$ ⁷, aortic peak Reynolds numbers in humans reach more
27 than twice^{8,9} this value, while in equine aortas peak values of 10 000 are common¹⁰. In the cardio-
28 vascular context, high turbulence levels constitute a severe health hazard, as intense fluctuations
29 and varying shear stresses are attributed to endothelial cell dysfunction and arteriosclerosis²⁻⁵.

30 In engineering applications, in addition to the excessive drag levels, fluctuations and alternat-
31 ing shear stresses can equally have adverse effects, and much effort has been dedicated to develop-
32 ing means to control turbulence. However, despite many novel and innovative approaches¹¹, so far,
33 a broadly applicable method remains elusive. Active control techniques¹²⁻¹⁴ require complex ac-
34 tuation devices^{15,16}, and in experimental realisations, the costs often far exceed the gains. Passive
35 approaches equally suffer from high implementation costs and typically have a limited operation
36 range^{1,17}. Additives, such as long chain polymers, degrade over time^{18,19} and contaminate liquids.
37 Available control techniques are hence problem specific and intrusive, requiring either manipula-
38 tion of fluid properties or costly and often impractical implementations. Conversely, aortic flow
39 provides an example where a specific propulsion scheme, consisting of impulsive bursts separated
40 by quiescent intervals, appears to hold turbulence at bay despite relatively large peak velocities.

41 The effect of unsteady, pulsatile driving on turbulence has been extensively investigated in
42 experiments and numerical simulations^{20–26}. In these studies, an initially steady turbulent flow
43 undergoes a periodic change in fluid speed, and the statistical properties of the evolving flow are
44 investigated. Flow acceleration typically delays turbulent kinetic energy production and decreases
45 the wall shear stress with respect to the quasi-steady value. Deceleration, on the other hand, en-
46 hances friction, although at higher deceleration rates, there is evidence of friction reduction²⁷.
47 Recent numerical studies^{28,29} identified unsteady driving conditions that can result in considerable
48 drag reduction, although the proposed numerical strategies are not necessarily straightforward to
49 implement in experiments in practice.

50 In this present study, we present an alternative approach to turbulence control, where drag
51 reduction is achieved by means of unsteady, pulsatile driving, specifically mimicking the cardiac
52 cycle and extending this method to large Reynolds numbers.

53 Experiments are carried out in a 1.2 m long pipe (inner diameter $D = 10$ mm), and water
54 is driven through the setup by a piston. The piston speed is accurately controlled by a servo
55 motor and allows us to alter the flow rate in time, and in particular, to realise a pulsatile flow of
56 the desired waveform. For further details of the experimental setup, we refer the reader to the
57 methods section . Initial experiments were carried out at moderate Reynolds numbers, values
58 which are comparable to those in aortic blood flow. We compare three flows in the same pipe set
59 up at identical instantaneous Reynolds number ($Re = U_m D / \nu$, where U_m is the instantaneous bulk
60 speed in the pipe). In the first case, the flow is driven steadily at $Re = 2\,800$ and as shown in Fig. 1a

61 the fluid motion is turbulent throughout. In the second experiment, the flow is driven periodically
62 using the waveform (see Fig. 1d) reported for cardiovascular flow in the descending part of a
63 human aorta³⁰, choosing a peak value close to the maximum values reported in literature³¹. Even
64 though the pipe set up is unchanged (including the inlet condition) the flow is fully laminar despite
65 instantaneous Reynolds numbers larger than 5000 (Fig. 1b) . We next tested a cycle in which the
66 diastolic rest phase was removed, as shown in Fig. 1 e. Compared to the cardiovascular case **d**,
67 we down-scaled the peak velocity by a factor of 1.5 so that the average Reynolds numbers of the
68 two cycles remain comparable. In this case, the flow indeed remains by and large turbulent, which
69 hints at the relevance of the diastolic rest phase for turbulence suppression.

70 From the above experiments, it is apparent that unlike for steady driving, the state of the
71 flow, i.e. laminar or turbulent, is not solely determined by the instantaneous Reynolds number
72 and that the waveform plays a decisive role. If turbulence develops during a cycle also depends
73 on the initial fluctuation level at the beginning of the cycle, and hence on the flow's history. In
74 this respect, the diastole plays a central role, as it effectively decouples the acceleration from the
75 prior deceleration, allowing turbulence and fluctuations to decay before Re increases again. In
76 the following, we investigate the effect of the pulsatile operation mode on a fully turbulent flow
77 at significantly larger time averaged Reynolds numbers $\overline{Re} = \overline{U}D/\nu$ (where \overline{U} is the bulk speed
78 averaged over one pulsation period, D the pipe diameter and ν the fluids kinematic viscosity) in
79 order to investigate the impact of pulsation on drag. To this end, we pump water through a 7 m
80 long pipe (inner diameter $D = 30$ mm) by means of the same syringe setup described above. The
81 pressure drop Δp is measured across a length $L = 120 D$ after a development length of $60 D$ from

82 the pipe inlet. Subsequently, the wall shear stress τ_w is reconstructed by using the force balance in
 83 the streamwise direction

$$\rho \frac{dU_m}{dt} = -\frac{\Delta p}{L} - \frac{4\tau_w}{D}, \quad (1)$$

84 where ρ is the water density and U_m is the instantaneous bulk flow velocity. Experiments are
 85 accompanied by direct numerical simulations (DNS) of the Navier–Stokes equations where the
 86 identical time variation of the Reynolds number is imposed. The DNS are performed for a 5D
 87 long pipe with periodic boundary conditions using a parallel solver³² (*NSPipeFlow*, see methods
 88 for further details).

89 In initial experiments and simulations, we tested a cycle consisting of a series of linear flow
 90 rate ramps smoothly joined together, corresponding to Re oscillating between $Re_{\min} = 3\,200$ and
 91 $Re_{\max} = 18\,800$ with a period $T = 4.5$ s, see Fig. 2 **a**. Note that, even for the minimum Re value,
 92 steady flows are fully turbulent in our pipe set-up.

93 From measurements of the pressure drop $\Delta p(t)$ and the imposed bulk velocity $U_m(t)$ we can
 94 determine the wall shear stress using equation (1). To ease comparison between different cycles, τ_w
 95 is nondimensionalized by the dynamic pressure at the cycles’ minima, corresponding to $(0.5\rho U_{\min}^2)$,
 96 where U_{\min} is the bulk velocity at $Re = 3\,200$. We hence define $\tau^* = 2\tau_w/(\rho U_{\min}^2)$ and in Fig. 2
 97 **d** the instantaneous experimental values (blue circles) are compared to the quasi–steady reference
 98 case, τ_{qs}^* (black dotted line), i.e. the wall shear stress expected if turbulence would instantaneously
 99 adjust to changes in Re . At the beginning of each cycle τ^* , although low, is considerably larger
 100 than τ_{qs}^* . Only as the flow acceleration proceeds measured values eventually fall below τ_{qs}^* , in line

101 with previous observations of drag reduction during flow acceleration.

102 While the instantaneous wall shear stress values indicate an overall drag reduction compared
103 to the quasi–steady case, this does not necessarily imply drag reduction compared to a steadily
104 driven flow of identical average Reynolds number. The drag change with respect to the steadily
105 driven flow is

$$R = \frac{\tau_{\text{steady}}^* - \overline{\tau^*}}{\tau_{\text{steady}}^*}, \quad (2)$$

106 where the overline denotes an average over several cycles, and the steady flow wall shear stress
107 τ_{steady}^* is obtained from the Blasius³³ friction factor relation and normalised in the same manner as
108 the cyclic flow. For the cycle of Fig. 2 **a**, the drag in experiments turns out to be 4.4% larger ($R =$
109 -0.044) than the steady flow. It is noteworthy that the quasi–steady case $\overline{\tau_{\text{qs}}^*}$ generally has a drag
110 considerably larger than the actual steady flow. In the present case it results in a 14% drag increase
111 compared to τ_{steady}^* . Pulsation hence does not necessarily lead to drag reduction let alone energy
112 saving. Inspired by the diastolic phase found in the aortic flow and the transition delay obtained
113 for the cardiac waveform, we designed a new cycle where a region of constant Re (rest phase) is
114 inserted that effectively decouples the deceleration from the consecutive acceleration phase (Fig. 2
115 **b**). Remarkably, the flow now responds with considerably lower values of τ^* during acceleration,
116 as well as during part of the deceleration phase (Fig. 2 **e**). The peak value of τ^* is reduced by a
117 factor of two, and in this case, we obtain a net drag reduction of 23% ($R = 0.23$). The central role
118 of the rest phase can be understood as follows. During acceleration, turbulence remains initially
119 frozen, i.e. variations in the mean velocity have a minimal impact on the turbulent stresses, leading
120 to significant drag reduction. The amount of drag reduction achievable sensitively depends on the

121 turbulence level at the beginning of this acceleration phase. Conversely, during deceleration, an
 122 inflection point emerges in the velocity profile, causing turbulence levels that typically exceed those
 123 expected for the instantaneous Re value, especially by the end of this phase. The subsequent rest
 124 phase crucially allows turbulence levels to die down and hence sets a favourable initial condition
 125 for the next acceleration phase.

126 From an energetic point of view, in unsteady flows a reduction of the mean friction τ^* is
 127 not sufficient to ensure that the power dissipation per unit length ($P = Q\Delta p/L$, where Q is the
 128 volume flow rate) is lower with respect to steady conditions. To quantify this aspect, we introduce
 129 the power saving

$$S = \frac{P_{\text{steady}} - \bar{P}}{P_{\text{steady}}}, \quad (3)$$

130 where P_{steady} is the power dissipated by the steadily driven, i.e. constant Re reference flow and \bar{P}
 131 is the time averaged power dissipation of the pulsatile flow. The instantaneous values of the power
 132 dissipation are given by $P(t) = \Delta p(t)Q(t)$, where $Q(t)$ is the volume flow rate, determined from
 133 the measured instantaneous piston speed. Computing the power savings for the cycle of Fig. 2 b
 134 yields a loss ($S = -0.03$), notwithstanding the large drag reduction. The power loss is caused by
 135 the additional energy input required to accelerate the flow, since an increase of flow rate requires
 136 the pressure gradient and hence the power to grow (cf. Eq. (1)). The waveform of Fig. 2b is hence
 137 advantageous (compared to steady driving) in situations where high shear stresses are detrimental,
 138 as is the case for the endothelium, but counterproductive if energy efficiency is the main incentive.
 139 While so far we have considered waveforms with lower acceleration and higher deceleration rates
 140 (Figs. 2 a and b), the opposite holds for velocity waveforms in the aorta³⁰. Correcting for this,

141 we chose the waveform displayed in Fig. 2 c, with a higher acceleration rate, while the rest phase
142 is left unchanged. During the more rapid Re increase, friction initially increases somewhat faster
143 than for waveform b, subsequently however, the friction drops at the beginning of the deceleration
144 phase (Fig. 2 f). Here, friction reaches levels comparable to the ones assumed during the rest
145 phase, albeit at very high Re . This effect further improves drag reduction, which now reaches 27%
146 ($R = 0.27$). Computing the power balance, we in this case obtain a net saving of 9% ($S = 0.09$)
147 compared to steadily driven pipe flow. Equally for the DNS, cycle Fig. 2 c is the only one that
148 results in drag reduction as well as energy saving. While the amount of drag reduction in the DNS
149 ($R = 0.28$) almost precisely matches experiments, the energy saving ($S = 0.07$) is slightly smaller.
150 Taking into account that due to computational cost, the DNS results were averaged over a much
151 smaller number of cycles, the agreement is nevertheless very good (see table Extended Data 2 and
152 Fig. Extended Data 3 for a comparison of experiments and DNS).

153 Finally, we investigate how changing the acceleration and rest phase affects drag reduction
154 and power savings. To this end, we carried out a total of 225 experiments spanning different rest
155 phase and acceleration durations (denoted respectively by T_r and T_a), while keeping minimum
156 and maximum Re and the combined duration of the acceleration and deceleration phases ($T =$
157 $0.02 \cdot 4\nu/D^2$) constant (cf. Fig. Extended Data 4). The resulting map of power saving S is shown
158 in Fig. 3 a.

159 The white, dashed line separates the regions of positive and negative S and the cycles of Fig.
160 2 a, b and c are denoted respectively by a circle, star and square. Interestingly, shorter acceleration

161 times consistently lead to higher power savings, hence suggesting the importance of a brief, intense
162 acceleration followed up by a longer, more gentle deceleration. Specifically for power saving we
163 find that the acceleration phase has to be much shorter ($\lesssim 1\%$) than the viscous time scales of
164 the flow. This abrupt change prohibits the flow profile's adjustment to its (high drag) quasi steady
165 shape. Strictly, for the parameter regime investigated, a non zero rest phase is required to save
166 power. However, there is an optimal rest phase and longer rest phases are counterproductive. The
167 optimal value of T_r depends weakly on T_a and it is approximately equal to half the duration of the
168 unsteady part of the cycle ($t \cdot 4\nu/D^2 \approx 0.01$). Remarkably, with $T_r^{\text{heart}} \cdot 4\nu/D^2 \approx 0.012$, the rest
169 phase observed for the aortic cycle in humans is close to this value.

170 The same parameter space can be mapped to the usual $f-\overline{Re}$ plane, where $f = 2D\Delta p/(\rho\bar{U}^2L)$
171 is the Darcy friction factor (Fig. 3 b), to highlight the effect of the cycles on the drag reduction R
172 and the dependence on \overline{Re} . For comparison, we plot the Blasius relation for turbulent friction. The
173 largest reduction in f (27% drag reduction) is found for $\overline{Re} \approx 8600$ and it is close to the region of
174 maximum S .

175 The circulatory system manages to combine flow speeds, significantly exceeding onset val-
176 ues of turbulence, with low shear stress levels. Sufficient flow rates are crucial for a functioning
177 organism, while at the same time, the stress levels have to remain tolerable for the blood vessels'
178 endothelial cell layer. As we have shown, the waveform of the cardiac cycle is close to optimal
179 to achieve both of these objectives. A rest phase during the cycle is crucial to diminish wall shear
180 stress and, at the same time, this rest phase has to be optimally timed and combined with a sub-

181 sequent rapid flow acceleration to not only reduce the flow drag but to also optimize its efficiency
182 and minimize power consumption.

183 Fluid transport is one of the largest sources of energy consumption in present day societies
184 and a major part of pumping costs can be attributed to turbulence. While pipeline flows are com-
185 monly run at a steady flow rate, our study demonstrates that, from an energetic point of view, this
186 is not necessarily the optimal operation mode.

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192 **Author Contributions**

193 B.H. supervised the project. D.S. and A.V. designed and performed the experiment. D.S. an-
194 alyzed the experimental data. J.M.L. designed and performed the computer simulations of the
195 Navier–Stokes equations and analysed the numerical results. D.S., J.M.L., A.V. and B.H. wrote
196 the paper.

197 **Author Information**

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199 no competing financial interests. Readers are welcome to comment on the online version of the
200 paper. Correspondence and requests for materials should be addressed to B.H. (bhof@ist.ac.at).

201 **References**

- 202 1. Kühnen, J. *et al.* Destabilizing turbulence in pipe flow. *Nat. Phys.* **14**, 386–390 (2018).
- 203 2. Davies, P. F., Remuzzi, A., Gordon, E. J., Dewey, C. F. & Gimbrone, M. A. Turbulent fluid
204 shear stress induces vascular endothelial cell turnover in vitro. *Proc. Natl Acad. Sci. USA* **83**,
205 2114–2117 (1986).
- 206 3. DePaola, N., Gimbrone, M. A., Davies, P. F. & Dewey, C. F. Vascular endothelium responds
207 to fluid shear stress gradients. *Arterioscler. Thromb. J. Vasc. Biol.* **12**, 1254–1257 (1992).
- 208 4. Davies, P. F. Hemodynamic shear stress and the endothelium in cardiovascular pathophysiol-
209 ogy. *Nat. Clin. Pract. Cardiovasc. Med.* **6**, 16–26 (2009).
- 210 5. Gimbrone, M. A. & García–Cardeña, G. Endothelial Cell Dysfunction and the Pathobiology
211 of Atherosclerosis. *Circ. Res.* **118**, 620–636 (2016).
- 212 6. Frenning, L. *Pump Life Cycle Costs: A Guide to LCC Analysis for Pumping Systems* (Hy-
213 draulic Institute, 2001).
- 214 7. Avila, K. *et al.* The Onset of Turbulence in Pipe Flow. *Science* **333**, 192–196 (2011).

- 215 8. Ku, D. N. *et al.* Blood flow in arteries. *Annual review of fluid mechanics* **29**, 399–434 (1997).
- 216 9. Stalder, A. F. *et al.* Assessment of flow instabilities in the healthy aorta using flow-sensitive
217 mri. *Journal of magnetic resonance imaging* **33**, 839–846 (2011).
- 218 10. Nerem, R. M., Rumberger Jr, J. A., Gross, D. R., Hamlin, R. L. & Geiger, G. L. Hot-film
219 anemometer velocity measurements of arterial blood flow in horses. *Circulation research* **34**,
220 193–203 (1974).
- 221 11. Brunton, S. L. & Noack, B. R. Closed-loop turbulence control: Progress and challenges.
222 *Applied Mechanics Reviews* **67** (2015).
- 223 12. Karniadakis, G. & Choi, K.-S. Mechanisms on Transverse Motions in Turbulent Wall Flows.
224 *Annu. Rev. Fluid Mech.* **35**, 45–62 (2003).
- 225 13. Min, T., Kang, S. M., Speyer, J. L. & Kim, J. Sustained sub-laminar drag in a fully developed
226 channel flow. *J. Fluid Mech.* **558**, 309–318 (2006).
- 227 14. Nakanishi, R., Mamori, H. & Fukagata, K. Relaminarization of turbulent channel flow using
228 traveling wave-like wall deformation. *Int. J. Heat Fluid Flow* **35**, 152–159 (2012).
- 229 15. Auteri, F., Baron, A., Belan, M., Campanardi, G. & Quadrio, M. Experimental assessment of
230 drag reduction by traveling waves in a turbulent pipe flow. *Phys. Fluids* **22**, 115103 (2010).
- 231 16. Kasagi, N., Suzuki, Y. & Fukagata, K. Microelectromechanical Systems-Based Feedback
232 Control of Turbulence for Skin Friction Reduction. *Annu. Rev. Fluid Mech.* **41**, 231–251
233 (2009).

- 234 17. Garcia-Mayoral, R. & Jiménez, J. Drag reduction by riblets. *Philos. Trans. R. Soc. Math.*
235 *Phys. Eng. Sci.* **369**, 1412–1427 (2011).
- 236 18. Virk, P. S., Mickley, H. S. & Smith, K. A. The Ultimate Asymptote and Mean Flow Structure
237 in Toms' Phenomenon. *J. Appl. Mech.* **37**, 488–493 (1970).
- 238 19. Choueiri, G. H., Lopez, J. M. & Hof, B. Exceeding the Asymptotic Limit of Polymer Drag
239 Reduction. *Phys. Rev. Lett.* **120**, 124501 (2018).
- 240 20. He, S. & Jackson, J. D. A study of turbulence under conditions of transient flow in a pipe. *J.*
241 *Fluid Mech.* **408**, 1–38 (2000).
- 242 21. Greenblatt, D. & Moss, E. A. Rapid temporal acceleration of a turbulent pipe flow. *J. Fluid*
243 *Mech.* **514**, 65–75 (2004).
- 244 22. He, S., Ariyaratne, C. & Vardy, A. E. Wall shear stress in accelerating turbulent pipe flow. *J.*
245 *Fluid Mech.* **685**, 440–460 (2011).
- 246 23. He, S. & Seddighi, M. Turbulence in transient channel flow. *J. Fluid Mech.* **715**, 60–102
247 (2013).
- 248 24. He, K., Seddighi, M. & He, S. DNS study of a pipe flow following a step increase in flow rate.
249 *Int. J. Heat Fluid Flow* **57**, 130–141 (2016).
- 250 25. Mathur, A. *et al.* Temporal acceleration of a turbulent channel flow. *J. Fluid Mech.* **835**,
251 471–490 (2018).

- 252 26. Cheng, Z., Jelly, T., Illingworth, S., Marusic, I. & Ooi, A. Forcing frequency effects on
253 turbulence dynamics in pulsatile pipe flow. *International Journal of Heat and Fluid Flow* **82**,
254 108538 (2020).
- 255 27. Ariyaratne, C., He, S. & Vardy, A. E. Wall friction and turbulence dynamics in decelerating
256 pipe flows. *J. Hydraul. Res.* **48**, 810–821 (2010).
- 257 28. Kobayashi, W., Shimura, T., Mitsuishi, A., Iwamoto, K. & Murata, A. Predic-
258 tion of the drag reduction effect of pulsating pipe flow based on machine learn-
259 ing. *International Journal of Heat and Fluid Flow* **88**, 108783 (2021). URL
260 <https://www.sciencedirect.com/science/article/pii/S0142727X21000138>.
- 261 29. Foggi Rota, G., Monti, A., Rosti, M. E. & Quadrio, M. Saving energy in turbulent flows with
262 unsteady pumping. *Scientific Reports* **13**, 1299 (2023).
- 263 30. Bürk, J. *et al.* Evaluation of 3D blood flow patterns and wall shear stress in the normal and
264 dilated thoracic aorta using flow-sensitive 4D CMR. *J Cardiovasc Magn Reson* **14**, 84 (2012).
- 265 31. Stein, P. D. & Sabbah, H. N. Turbulent blood flow in the ascending aorta of humans with
266 normal and diseased aortic valves. *Circulation research* **39**, 58–65 (1976).
- 267 32. López, J. M. *et al.* nscouette – a high-performance code for direct numerical sim-
268 ulations of turbulent taylor–couette flow. *SoftwareX* **11**, 100395 (2020). URL
269 <https://www.sciencedirect.com/science/article/pii/S2352711019302298>.
- 270 33. Blasius, H. Das Ähnlichkeitsgesetz bei Reibungsvorgängen in Flüssigkeiten. *Mitteilungen*
271 *Über Forschungsarbeiten Auf Dem Geb. Ingenieurwesens* **131** (1913).

272 34. Tanaka, M., Girard, G., Davis, R., Peuto, A. & Bignell, N. Recommended table for the density
273 of water between 0 C and 40 C based on recent experimental reports. *Metrologia* **38**, 301
274 (2001).

Figure 1: Decay of turbulence in aortic flow. Panel **a** to **c** show three instantaneous snapshots of flows at $Re = 2800$. Images capture flow structures in a $30D$ long area located $60D$ downstream of the pipe inlet. In **a** the flow is driven steadily and Re is hence constant. In **b** and **c** flows are driven periodically respectively with **(b, d)** and without **(c, e)** a diastolic rest phase. For the periodic waveforms, the minimum Reynolds number is $Re_{\min} = 270$ in **d** and $Re_{\min} = 180$ in **e**, while the maximum value is $Re_{\max} = 5300$ in **d** and $Re_{\max} = 3500$ in **e**. The cycle averaged values correspondingly are $\overline{Re} = 1730$ for **d** and $\overline{Re} = 1890$ for **e**.

Figure 2: Friction reduction in pulsating flow. Effect of three different cycles on the wall shear stress. In all cases $Re_{\min} = 3200$ and $Re_{\max} = 18800$. In **a** $\overline{Re} = 11000$, in **b** and **c** $\overline{Re} = 8600$. The corresponding Reynolds number modulation is imposed in experiments and in direct numerical simulations. Panels **d**, **e** and **f**, display the measured dimensionless wall shear stress τ^* for experiments (blue circles) and DNS (red line). For comparison, the friction associated with the quasi-steady flow is provided by the black dotted line. The quasi-steady values are given by $\tau_{qs}(t) = 0.079Re(t)^{-0.25}U_m(t)^2/U_{\min}^2$ (where the Blasius friction scaling is assumed).

Figure 3: Optimization of power savings. **a** Percentage of the power savings S as a function of the duration of the acceleration T_a and rest phase T_r . The white, dashed line separates the region of positive and negative S . The circle, star and square represent the parameters for the cycles of Fig. 2 **a**, **b** and **c**, respectively. **b** corresponding values of S represented in the traditional $f-Re$ plane, where $f = 2D\Delta p/(\rho\bar{U}^2L)$ is the Darcy friction factor. The gray dashed line is the friction level of a steady turbulent flow (Blasius correlation).

275 Methods

Direct numerical simulations We solve the incompressible Navier–Stokes equations in cylindrical coordinates in a pipe of length $5D$ with periodic boundary conditions at the extremities. The equations are written in non–dimensional units by using the pipe radius, $D/2$, as the length scale, the viscous time, $(D)^2/(4\nu)$, as the time scale, and $2\nu/D$ as the velocity scale. They take the following form:

$$\partial_t \mathbf{u} + (\mathbf{u} \cdot \nabla) \mathbf{u} = -\nabla p + \nabla^2 \mathbf{u}, \quad (4)$$

$$\nabla \cdot \mathbf{u} = 0, \quad (5)$$

276 To impose a time–varying Reynolds number, the mean velocity is updated at every time step,
277 namely

$$U_{m,\text{new}} = U_{m,\text{old}} + \alpha(t)\delta t, \quad (6)$$

278 where δt is the time step and $\alpha(t)$ is a prescribed acceleration rate. An axial forcing term is then
279 added to the Eq. (4) to enforce that the integral of the instantaneous velocity profile yields the
280 mean flow, *i.e.*

$$U_m = \int_0^1 2u(r)r dr. \quad (7)$$

281 Simulations were carried out by using the custom, highly–scalable, pseudo–spectral solver
282 *NSPipeFlow*. The codes employs Fourier–Galerkin expansions along the axial and azimuthal
283 directions, and eighth–order, finite central differences for the radial dimension, collocated on a
284 Gauss–Lobatto–Chebyshev grid. The equations evolve in time with a second–order, predictor–

285 corrector algorithm and a time step dynamically adjusted to satisfy the Courant–Friedrich–Lewy
286 condition. Typical values of the time step size in our simulations range from 10^{-8} to 10^{-10} viscous
287 units. For further details about the code implementation, we refer the reader to Lopez *et al.* ³².
288 As the Reynolds number changes over time by more than an order of magnitude, the code can
289 adaptively change the grid spacing to match the required spatial resolution needs. More specifi-
290 cally, the adaptive grid method we have implemented ensures that the spatial resolution in the axial
291 and azimuthal directions is consistently below 7.5 wall units, whereas the maximum and minimum
292 spacing in the radial direction is below 3 and 0.1 wall units, respectively. This spatial resolution
293 is more stringent than that customarily used in DNS studies of pipe flow at steady Reynolds num-
294 bers. Typical values found at the minimum and maximum Reynolds numbers are given in Table
295 Extended Data 1.

296 The number of cycles needed to achieve statistical convergence depends on the pulsation
297 waveform. For the case shown in Fig 2d, cycles have little variation, and convergence occurs fast.
298 Statistics were computed in this case using four cycles. For the cases shown in figures 2e y f,
299 there is more variability among cycles, and it is necessary to average over more cycles to obtain
300 converged statistics. For the waveform shown in Fig 2e, statistics were obtained averaging over
301 nine cycles, whereas, for the waveform shown in Fig 2f, 14 cycles were used.

302 **Experimental set-up** We employ a large scale, customized syringe pump (sketched in Fig. Ex-
303 tended Data 1) to control precisely the flow rate and hence impose an arbitrary modulation of
304 the Reynolds number. The test section consists of a 7 m long, precision bore glass pipe (Duran,

305 KPG, internal diameter $D = 30 \pm 0.01$ mm) made by joining 1 m long segments with custom
306 PMMA flanges (in the experiments of Fig. 1 the test section consists of a single pipe segment with
307 $D = 10 \pm 0.01$ mm and length 1.2 m). Water flows through the pipe into a reservoir as the syringe
308 pump is displaced by a linear actuator driven by a servomotor (Festo, ESBF-BS-80-1500-15P and
309 Festo, EMMS-AS-70-M-LS-RS, not shown in Fig. Extended Data 1). A PC is used to control the
310 motor and thus the plunger speed within an accuracy of ± 0.01 mm/s. The syringe has an inter-
311 nal diameter of $D_c = 125 \pm 0.11$ mm and total length $L_c = 1500 \pm 0.1$ mm, corresponding to a
312 maximum run time of ≈ 870 advective time units (D/U) for the chosen pipe diameter. Turbulence
313 development is ensured by perturbing the flow at the pipe inlet with a pin and letting the flow
314 develop for $60 D$. Differential pressure is measured over the subsequent $120 D$ with a carefully
315 calibrated pressure transducer, full scale 2.5 kPa. The wall taps (diameter $d = 0.5$ mm) are drilled
316 through the PMMA flanges and have been polished to remove any burr. Water temperature is mon-
317 itored at the outlet of the pipe with a Pt-100 probe (indicated as T in Fig. Extended Data 1) and
318 typically is held constant within ± 0.05 °C. In a typical measurement run the desired flow rate wave
319 form is repeated cyclically while traversing the available stroke length. Temperature is measured
320 in real-time in order to compute the correct motor speed and hence imposing the correct Reynolds
321 number. The control and acquisition frequency are set to 50 Hz. Depending on the period duration
322 single runs consists of between 10 and 12 cycles. To ensure a proper statistical representation of
323 the unsteady friction each run is then repeated several times (100 times for the results of Fig.2 and
324 50 times for the parametric study of Fig.3). The pressure signal has been filtered to attenuate os-
325 cillations due to setup vibrations by using a cutoff frequency of 5Hz. The first cycle is found to be

326 systematically different from the others it has been excluded from the averaging process. Overall,
327 the drag reduction R and the power savings S are estimated with a $2\text{-}\sigma$ accuracy of $\pm 1.8\%$ and
328 $\pm 2.2\%$, respectively.

329 **Calibration** In order to ensure repeatable and accurate differential pressure measurements we
330 calibrate the pressure sensor immediately before starting a batch of measurements (a typical batch
331 consists of 10 runs with a minimum of 10 cycles each). For the calibration we measure the pressure
332 drop along the test section Δp for five values of the Reynolds number Re . Each steady measure-
333 ment is repeated five times and the values of Δp , the piston speed in the cylinder U_c and water
334 temperature T are recorded. The reference value of Δp is computed for each Re by using the
335 Blasius formula,

$$\Delta p = 0.316 Re^{-0.25} \frac{1}{2} \rho U^2 \frac{L}{D}, \quad (8)$$

336 where $U = U_c D_c^2 / D^2$ is the flow mean velocity in the pipe, D_c is the diameter of the cylinder, L
337 is the length of the test section and ρ is the density of water derived from the temperature T by
338 following the procedure described in ³⁴. As a result, a calibration curve is obtained to convert the
339 sensor output (in Volts) to a differential pressure in Pascal. To assess the validity of the calibration
340 we compute the residuals of the linear fit and take the maximum value. In the case of the optimal
341 cycle (Fig. 2, **c** and **f**) we find a maximum deviation of ≈ 10 Pa, which is well representative of
342 the values found throughout the experimental campaign.

343 **Standard deviation of mean pressure and flow rate measurements.** The mean pressure drop
344 during a cycle is estimated by taking the sample average of the signal $\Delta p(t)$, namely

$$\overline{\Delta p} = \frac{1}{N} \sum_{i=1}^N \Delta p_i, \quad (9)$$

345 where Δp_i is the i -th sample $\Delta p(t_i)$ and N is the number of samples per cycle. The pressure
346 signal recorded for the optimal waveform is reported in Fig.Extended Data 2 **b**. The blue curves
347 correspond to 100 instantaneous cycles and the phase average is shown in red. For comparison we
348 superimpose the computed pressure drop from DNS (dotted line). (Fig.Extended Data 2 **a** shows
349 the corresponding time dependence of the Reynolds number based on the recording of the piston
350 position).

351 Using Eq.(9) we determined the mean pressure for all 100 cycles and found that the standard
352 deviation between cycles amounts to 2.9% of the mean. This value provides an upper bound on
353 the measurement error involved. Here it has to be taken into account that, due to the unsteady,
354 chaotic nature of the flow consecutive cycles start from different initial conditions, which leads
355 to a natural variation of cycle averaged quantities such as mean pressure. Hence the standard
356 deviation between cycles would be expected to be non-zero even in the absence of measurement
357 error. The error of the mean flow rate \overline{Q} can be estimated from positioning measurements of the
358 piston and the manufacturing accuracy of the piston cylinder, to be 0.6%. For the power input
359 curves, Fig.Extended Data 2 **c**, the standard deviation surmounts to 3.1% .

360 **Computing drag reduction from experimental measurement** The drag reduction rate R can be
361 computed by integrating Eq. (1) integer multiples of the period T of the waveform.

$$\int_0^{mT} \rho \frac{dU(t)}{dt} dt = - \int_0^{mT} \left(\frac{\Delta p(t)}{L} + \frac{4\tau_w(t)}{D} \right) dt, \quad (10)$$

362 where we assume incompressible flow and make use of the fact that the integral of the bulk flow
 363 over a period is zero

$$\int_0^{mT} \frac{\Delta p(t)}{L} dt = - \int_0^{mT} \frac{4\tau_w(t)}{D} dt, \quad (11)$$

364 We can therefore rewrite Eq. (2) to express the drag reduction rate R in terms of the time averaged
 365 pressure and hence

$$R = \frac{\Delta p_{\text{steady}} - \overline{\Delta p}}{\Delta p_{\text{steady}}}, \quad (12)$$

366 where Δp_{steady} is computed for the mean Reynolds number \overline{Re} of the cycle by using the Eq. (8).

367 As a consequence, the standard deviation in $\overline{\Delta p}$ (2.9% in case of the optimal cycle) provides
 368 an upper bound for the uncertainty in R .

369 **Estimation of the power saving** Estimating S is also quite straightforward, as it requires taking
 370 time averages of the power $P(t) = \Delta p(t)Q(t)$, where $Q(t)$ is the volume flow rate and using Eq.(3,
 371 main text), reported here for clarity:

$$S = \frac{P_{\text{steady}} - \overline{P}}{P_{\text{steady}}}. \quad (13)$$

372 The accuracy of S can be estimated in the same way we described for R . We compute the mean
373 power \overline{P} for each of the 100 cycles and then estimate the standard deviation between the cycles.
374 We find a value of 3.2%, which also represents of the accuracy of S since in Eq.(13) \overline{P} is the only
375 uncertain quantity.

376 **Comparison with DNS** Selecting the optimal waveform (Fig. 2c) we compare the values of R
377 and S obtained from experiment to those observed in direct numerical simulations. The histograms
378 of the 100 cycles measured experimentally are shown in Fig. Extended Data 3 (a) and (b). Since
379 (due to computational costs) a much smaller number of cycles have been simulated, instead of
380 histograms, we computed the mean values for the DNS for R and S (orange dashed lines).

381 Finally, we report in table Extended Data 2 the average values for R and S for all three
382 waveforms of Fig. 2 for experiments and DNS and they turn out to be in close agreement.

383 **Waveforms** The waveforms considered are composed of linear ramps in Re and periods of con-
384 stant flow rate. Throughout the experiments the minimum and maximum Re are held constant and
385 equal to $Re_{\min} = 3\,200$ and $Re_{\max} = 18\,800$, respectively. The combined duration of acceleration
386 and deceleration T is always fixed to 4.5 s, while the duration of the acceleration and rest phase are
387 respectively varied in the intervals $T_a \in [1.35, 3.15]$ s and $T_r \in [0, 4]$ s. To avoid abrupt changes
388 in the piston acceleration, the sudden slope changes, that occur at the transition points from accel-
389 eration to deceleration to rest phase, have been locally smoothed with a moving average filter of
390 width 0.8 s (cf. Fig. 2 (a), (b) and (c)).

391 **Data availability**

392 The datasets generated and analyzed during the current study are freely available in the Zenodo
393 repository, <https://doi.org/10.5281/zenodo.7828996>.

394 **Code availability**

395 The numerical simulations were conducted with the open source code nsPipeFlow, distributed un-
396 der the terms of the GNU General Public License version 3. A detailed description of the code and
397 user guide is provided in reference 30. The code version used in this study and an initial condition
398 to start the simulations are openly available in the Zenodo repository, <https://doi.org/10.5281/zenodo.7828996>.

Figure Extended Data 1: Sketch of the experimental setup. Drawing not to scale.

Figure Extended Data 2: Waveform, pressure and power signal. Signals from the optimal cycle (Fig. 2c) measured in experiments. (a) Waveform based on the linear piston speed and (b) pressure drop Δp measured over the test section. The signal from all the 100 cycles measured is shown in blue, while the phase average is represented in orange. The number of samples per cycles is $N = 325$. For comparison, we report also the pressure drop computed with the DNS for the same cycle (gray dotted line). In this case the signal is obtained by phase-averaging the available 8 cycles. (c) The power input for the same waveform. The values for the 100 cycles in experiments are shown in blue, the ensemble average in red and the power input in DNS is given by the grey dotted line.

Figure Extended Data 3: Comparison of the values of (a) R and (b) S between experiments (blue histogram) and DNS. For the optimal cycle (Fig. 2c, main text) the histogram shows the distribution of the values obtained from 100 runs. The orange, dashed line shows the mean of the available corresponding DNS cycles.

Figure Extended Data 4: Definition of the flow cycle used in the experiments of Fig.2 and Fig.3.

Table Extended Data 1: Parameters used in the direct numerical simulations. From left to right: Reynolds number Re based on the mean velocity, minimum and maximum radial resolution (in inner units), azimuthal resolution (in inner units), axial resolution (in inner units) and average time step size δ_t .

Table Extended Data 2: Comparison between the values of R and S in percentage for the waveforms of Fig.2 obtained from experiments and DNS.