

Title	A Three-Dimensional Cell Culture Platform for Long Time-Scale Observations of Bio-Nano Interactions	
Authors(s)	Muraca, Francesco, Alahmari, Amirah, Giannone, Valeria A., Adumeau, Laurent, Yan, Yan, McCafferty, Mura M., Dawson, Kenneth A.	
Publication date	2019-11-04	
Publication information	Muraca, Francesco, Amirah Alahmari, Valeria A. Giannone, Laurent Adumeau, Yan Yan, Mura M. McCafferty, and Kenneth A. Dawson. "A Three-Dimensional Cell Culture Platform for Long Time-Scale Observations of Bio-Nano Interactions" 13, no. 11 (November 4, 2019).	
Publisher	ACS	
Item record/more information	http://hdl.handle.net/10197/12162	
Publisher's statement	This document is the Accepted Manuscript version of a Published Work that appeared in final form in ACS Nano, copyright © 2019 American Chemical Society after peer review and technical editing by the publisher. To access the final edited and published work see http://pubs.acs.org/doi/abs/10.1021/acsnano.9b07453.	
Publisher's version (DOI)	10.1021/acsnano.9b07453	

Downloaded 2023-10-06T13:54:56Z

The UCD community has made this article openly available. Please share how this access benefits you. Your story matters! (@ucd_oa)



© Some rights reserved. For more information

A three-dimensional cell culture platform for long time-scale observations of bio-nano interactions

3 Francesco Muraca^a, Amirah Alahmari^a, Valeria A. Giannone^{a,b}, Laurent Adumeau^a, Yan

4 Yan^{a,b}, Mura M. McCafferty^{a*}, Kenneth A. Dawson^{a*}

5 a: Centre for BioNano Interactions, University College Dublin, Belfield, Dublin 4; b: School

6 of Biomolecular and Biomedical Science, University College Dublin, Belfield, Dublin 4.

* kenneth.a.dawson@cbni.ucd.ie, mura.mccafferty@cbni.ucd.ie: Correspondence should be
addressed to these authors.

9

10 SUMMARY

We know surprisingly little about the long-term outcomes for nanomaterials interacting with 11 12 organisms. To date, most of what we know is derived from *in vivo* studies that limit the range 13 of materials studied, and the scope of advanced molecular biology tools applied. Long-term in vitro nanoparticle studies are hampered by a lack of suitable models, as standard cell culture 14 techniques present several drawbacks, while technical limitations render current 3D cellular 15 16 spheroid models less suited. Now, by controlling the kinetic processes of cell assembly and division in a non-Newtonian culture medium, we engineer reproducible cell clusters of 17 18 controlled size and phenotype, leading to a convenient and flexible long-term 3D culture that 19 allows nanoparticle studies over many weeks in an in vitro setting. We present applications of this model for the assessment of intracellular polymeric and silica nanoparticle persistence, and 20 21 found that hydrocarbon based polymeric nanoparticles undergo no apparent degradation over long time periods with no obvious biological impact, while amorphous silica nanoparticles 22 degrade at different rates over several weeks, depending on their synthesis method. 23

Keywords: 3D cell culture, cell cycle, quiescence, bio-nano interactions, nanoparticle
persistence, nanoparticle degradation, silica nanoparticles

Nanostructures can gain access to biological (intracellular and other) compartments where they may accumulate and slowly degrade, producing various by-products.¹⁻⁴ This differs from the more familiar scenarios of small molecules having short *in situ* cellular half-lives, or macroscopic material implants exposed to extracellular degradation, so it is unclear what can be learned about the fate of particles by analogy to those situations.

32 Broadly speaking, nanoparticle populations present diverse biomolecular surfaces leading to 'scattergun' interactions with various cells, tissues and organs (including the liver).^{5–12} There 33 they will be incorporated and processed within endogenous intra- and trans-cellular trafficking 34 pathways;^{13–15} however, instead of being cleared rapidly, they may be retained for extended 35 periods of weeks, months, or longer.^{16–19} This could lead to persistent signalling dysregulation 36 37 or other adverse biological processes, and the slow degradation of the particle to secondary (and other downstream) metabolites.^{20–24} Given this diversity of interaction modalities, in early 38 explorations it was surprising for some that few detrimental biological effects were observed 39 for 'passive' materials, not otherwise chemically toxic. Still, it must be emphasised that much 40 of what we currently know comes from short-term in vitro cell-level studies extending over 41 hours,^{21,25-29} with limited information on the consequences of longer-term intracellular 42 nanoparticle localisation. This is primarily due to a lack of suitable *in vitro* models to address 43 this issue, as commonly used cell culture systems fail to capture the complex in vivo 44 45 environment, and are unsuitable for long-term nanoparticle studies due to rapid dilution of the intracellular nanoparticle load by cell division.^{30,31} Thus, with the exception of a few studies 46 that apply cell spheroids,32-36 the little information available on long-term particle 47 48 accumulation, degradation and cellular responses is largely observational and limited in scope, being derived from specialised in vivo studies.^{19,23,37–40} 49

Rather topical examples where simplified models could shed some highly desirable light on their long-term impacts include polymeric and silica nanoparticles. Polymeric nanoparticles are either manufactured, or result from degradation of bulk polymers in the environment, and silica nanoparticles are widely used in industrial processes. Currently, the systematic study of these issues (without the use of animals), is essentially blocked.

Here we describe a highly reproducible, long-term three-dimensional (3D) culture model of 55 small cellular assemblies that possess the architecture and some *in vivo* phenotypical features 56 that are particularly suitable for studying long-term nanoparticle exposure. They may be 57 created using immortalized cell lines, without the deficits suffered by dividing cells. As these 58 59 cell clusters assemble, they re-form inter-cellular junctions, and restore functions known to 60 predominate in the native tissue. Moreover, the cells transition to a quiescent state, while 61 remaining metabolically active, thereby avoiding the confounding effects of cell division. The architecture of these assemblies is well defined, and the arrangement of cells is such that most 62 are accessible to the cluster surface, ensuring viability over many weeks and months. These 63 64 cell clusters possess ideal characteristics for studying the long-term effects of nanoparticle exposure in vitro, and are applied here for the assessment of polymeric and silica nanoparticles 65 66 over several weeks.

67

68 **Results**

Long-term cell cluster architecture for nanoparticle exposure: We grow controlled cell clusters by suspension of dividing cells in a non-Newtonian polymeric additive (hereafter referred to as suspension media) that acts as a low viscosity liquid at shorter length and motional timescales, while damping motion at longer length and time scales. This allows for diffusion of nutrients and nanoparticles, while whole-cell motion is slow and multi-cell motion is essentially quenched. While attempts to improve control of cell cultures using the viscoelastic

properties of media have been discussed previously,⁴¹ our exploration suggests this may be an 75 important dimension in the creation of organoid-like structures in future. There are numerous 76 77 approaches to achieving control over culture media viscosity at the different length scales (tens 78 of nanometres to micron). Soft-gelling polymer complexes have the convenience that they are 79 readily optimised by dilution, small changes of ionic strength or other simple experimental control parameters. Examples we have explored include an enzyme modified galactomannan 80 (Guar gum) and xanthan blend additive.⁴² There are many ways of achieving similar relevant 81 viscoelastic responses, so for simplicity our results are based on a standardised and widely 82 83 available formulation.

By tuning the viscoelastic properties of the suspension media, we can control the reproducible 84 85 formation, and structural and functional evolution of small cell clusters. Besides the 86 fundamental issue of cell growth and assembly kinetics (about which we still have much to learn), there are also other practical optimisations, such as the avoidance of cell dropping or 87 attachment to the bottom of the plates by applying an agar coating before cell seeding in the 88 suspension media (Figure 1a). A549 human lung epithelial cells have been used for the work 89 90 presented here, and we also report the possibility to reproduce these characteristics with other 91 cell lines (Supplementary Figure S1).

92

93 *Cluster growth kinetic stages:* The basic kinetic processes of cell cluster formation are deduced 94 from different regimes of time-lapse microscopy captured over 5 days (Supplementary Videos 95 1-7), with more detailed imaging and analysis used to follow the outcome in a quantitative 96 manner. Early on, single 'itinerant' cells within the medium can move relatively short distances 97 and divide; therefore, during the first several days, cell-cell associations primarily arise from 98 engagement (collision) of nearby cells, and cell division. During this 'core formation' stage 99 some cells engage briefly before continuing to move while others attach, leading to small core 100 clusters of two or three cells, after which, adjustments of cluster shape take place. After twenty-101 four hours there is progressive crossover to the second 'cluster-maturation' kinetic stage in 102 which the (near-stable and increasingly immobile) 'core' clusters grow, partly via collision 103 with itinerant cells and proximate small clusters, and partly by division of cells within the 104 cluster (Supplementary Figures S2, S3). We also observe other rarer processes; for example, a 105 cell (or two) that lies between two neighboring clusters can form a bridge between them to promote their merger. 'Cluster stabilisation' commences around day five, wherein most of the 106 itinerant cells are exhausted, rapid cluster growth ends, and established clusters are essentially 107 108 immobile (Figure 1b).

109 Cluster size and shape evolution: The distribution of the major (long) axis length of the 110 growing and maturing clusters exhibits a tail and is therefore not strictly Gaussian (Figure 1c, 111 Supplementary Figure S4 and Supplementary Table S1). While the origin of this small proportion of larger cluster size is not yet fully understood (it could be due to some cells 112 113 reaching the agar-coated surface and forming slightly larger structures), if we extract a median 114 or mean size from the distributions over time, the most rapid cluster size increase indeed accompanies the cluster growth stage, and changes slow dramatically after the first five days 115 (Figure 1d). At the cluster stabilisation stage, the minor axis begins to be approximately 116 described as a bilayer of cells. The fact that clusters are restricted in size (typically less than 117 100 µm; Figure 1c-e and Supplementary Figure S4) and oblate in shape (Figure 1f and 118 119 Supplementary Figure S5) means that most cells have access to nutrients, gas supply and waste clearance,⁴³ and thus remain viable throughout the culture time (Supplementary Figure S6). 120 The clusters can be easily isolated and used for many practical purposes after the first week in 121 122 culture.

Evolution of nanoparticle-relevant cellular function accompanying cluster growth: While there are many changes in cell morphology, ultra-structure, function and phenotype occurring 125 during cluster formation, it is not always clear to what degree they drive, or are a consequence of, multi-cell assembly. A broad proteomics screening comparing A549 clusters with the same 126 cells grown as monolayer revealed major changes in the phenotype of the clusters. There is a 127 128 shift toward a quiescent, secretory phenotype after the first week of culture (Supplementary Figures S7, S8, S9). Moreover, an increase in ROS defence coupled with increased 129 mitochondrial activity and fatty acid metabolism suggests that a deep metabolic alteration, 130 consisting of a shift toward a more ROS resistant phenotype, is occurring within the clusters in 131 suspension.44,45 132

Cell-cell adhesion is fundamental for the stability of biological tissues, providing structural rigidity and other functional cues.⁴⁶ Compared to monolayer cells where the main cell interactions occur with the culture substratum, the clusters form strong cell-cell interactions immediately upon contact.⁴⁷ E-cadherin mRNA expression is upregulated in cells organised in clusters in the suspension media compared to monolayer grown cells, and the protein is more strongly presented at the cell surface and interface, consistent with cell-cell adhesion complex formation (Figure 2a-c and Supplementary Figure S10).

140 With the formation of clusters, an increase in cell secretory events was observed. There is a significant increase of mucin 5AC and IgG Fc binding protein mRNA expression in the cell 141 142 clusters compared to monolayer, and wheat germ agglutinin (WGA) staining revealed a thickening and rearrangement of surface carbohydrate residues containing sialic acid and N-143 acetylglucosamine residues, consistent with increased respiratory mucus secretion⁴⁸ (Figure 144 145 2d-g, and Supplementary Figure S11). TEM micrographs of clusters confirm that there are 146 numerous secretory granules and vesicles within the cells after the first week of culture, with secretion of different materials (Figure 2h,i and Supplementary Figure S12). Additionally, 147 148 some lysosomal activities seem to be differently regulated in the clusters, with increased expression of cathepsins and other important transcription factors, which could be related to 149

extracellular matrix remodelling (Supplementary Figure S13). Taken together, these results indicate that the A549 cell clusters grown in this way possess characteristics that more closely represent their native *in vivo* phenotype, compared to the same cells cultured in monolayer.

Nanoparticle uptake, dilution, and trafficking in dividing and quiescent cell states: 153 Traditionally, understanding the uptake and trafficking of nanoparticles in monolayer cells is 154 155 complicated by the fact that upon division, cells split their intracellular contents between daughter cells, thereby diluting the nanoparticle load. Therefore, the establishment of a 156 quiescent state in the cells organised as clusters is critical for the long-term assessment of 157 158 nanoparticle interactions. A time-resolved cell cycle analysis of the clusters determined that all 159 but the G0/G1 phases are depopulated during the first week (Figure 3a, b and Supplementary 160 Figures S14, 15). After two weeks there are no cells in the S phase, while cell viability remains largely unaffected. Furthermore, p27kip1 (a G1 cyclin complex inhibitor critical in the 161 162 maintenance of quiescence⁴⁹) mRNA expression is increased (Figure 3c). Consistent with this 163 finding, Ki67 antigen (a proliferative cell marker) mRNA and protein expression is almost 164 completely downregulated in matured clusters (Figure 3d, e, f, and Supplementary Figure S16). Together, these results suggest that the cells have exited the cell cycle and entered the quiescent 165 (G0) phase. When cells are recovered by disassembly of the clusters and reconstituted into 166 monolayer, they rapidly restore normal cell cycling, even after up to 3 weeks of cluster culture 167 (Supplementary Figures S17, 18). We therefore believe that the cell clusters have established 168 169 a quiescent state, which (given the intrinsic limitation of using rapidly dividing cells) is more 170 useful for application in long-term nanoparticle studies.

For the cluster model presented here, cells can be exposed to particles either prior to or after formation of clusters, and the outcomes studied over many weeks (during which the cells are in their quiescent state). We present results for these exposure scenarios using polystyrene carboxylate-modified nanoparticles (PS-COOH NPs), conventionally considered non175 degradable and non-toxic. For the pre-cluster formation exposure method (Figure 4a), cells in 176 monolayer were exposed to particles for 4 hours (0.1 mg/mL), then seeded in the suspension media to form clusters. Within the first days of cluster culture, the nanoparticle fluorescence 177 178 loss is reduced, and after several days there is little further decrease. Indeed, for some weeks thereafter there is no significant change in the quantity of nanoparticles in cells in clusters nor 179 180 any evident cell cycling, while the dividing monolayer cells have lost their nanoparticle population due to dilution (Figure 4b, c, d and Supplementary Figures 19). Confocal 181 182 microscopy imaging suggests that most particles remain localised within lysosomes during 183 those extended periods (Figure 4e and Supplementary Figure 20).

Significantly, this model allows for another exposure scenario, in which living quiescent 184 185 suspended cell clusters can be treated directly with nanoparticles (Figure 4f). Clusters (grown 186 for 1 week) were treated in the suspension environment with 0.02 and 0.1 mg/mL PS-COOH NPs for 4 hours, and a higher uptake was observed for both particle concentrations, in 187 comparison with monolayer cells (Figure 4g, h, i and Supplementary Figures S21, 22). While 188 189 there is still much to be learned about nanoparticle uptake and trafficking in these clusters, one 190 key observation is that most cells in the cluster are exposed to particles, although at different levels, seemingly irrespective of their location (Figure 4 j, k, l, m, and Supplementary Figures 191 192 S22, 23). Immediately after nanoparticle treatment, some particles can be seen on the surface of the cells, especially at the mucus interface (Figure 4i, k); however, 24 hours after treatment, 193 194 particles are no longer observed on the surface of the clusters (Figure 41, m). The fact that many 195 particles are present even in cells that seem to have their external surface completely covered 196 with mucus suggests that nanoparticles can reach the cell membrane and be internalised, even 197 in the presence of thick mucus layers. Also, as most cells are already in their quiescent state 198 when treated, there is little dilution of nanoparticles due to cell division, even after many weeks (Supplementary Figure S24). The minimal loss of particles from the cell clusters is an expected, 199

but significant, confirmation that much of the apparent dilution of intracellularly accumulated particles observed in recent years is indeed directly related to cell division.³⁰ These results also give us a first opportunity to meaningfully investigate the long-term consequences of intracellular nanoparticle accumulation.

Modelling long-term nanoparticle exposure and degradation scenarios: While it is not our 204 205 intention here to report on exhaustive studies of long-term nanoparticle exposure, it is clear that the quiescent cluster model will allow a detailed mechanistic insight into the evolution of 206 207 nanoscale materials inside living organisms. Using the exposure system described above, we 208 illustrate the potential for valuable outcomes using examples of different types of silica nanoparticles, a material of significant practical interest. While silica has long been considered 209 210 biodegradable in biological milieu, it is less well understood that this question is a matter of 211 the material structure (dictated by the synthesis processes), as well as the details of its specific cellular localisation. We illustrate this using two different forms of silica: SiO₂ – an amorphous 212 silica nanoparticle, and $SiO_2(a)SiO_2$ – an amorphous silica nanoparticle coated with an 213 214 additional, more dense layer of silica (Supplementary Figure S25).

215 Both formulations of SiO₂ particles show extensive degradation in biological cell culture media (cMEM), while there is little or no degradation in artificial lysosomal fluid (ALF) (Figure 5a). 216 Accumulation in the cell lysosomes in quiescent clusters leads to slow degradation over many 217 weeks (Figure 5b and Supplementary Figure S26, 27). The SiO₂ particle shows a higher degree 218 219 of degradation within the lysosomes, as changes in the surface of the particle are observed, 220 together with a decrease in particle size. Indeed, by 4 weeks in culture, some of the particles are significantly degraded with a distinct architecture no longer visible. In contrast, the 221 SiO₂@SiO₂ particles remain stable in the lysosomes for longer, with minimal changes in shape 222 and size by the end of the 4 week culture period (although some etching of the surface can be 223 observed). In no case do we observe any significant biological impacts on the cultures, even 224

when the silica slowly degrades, and currently we believe that most (amorphous) silica will
degrade over quite long periods, dependent on the specific nature of the material.

The contrast with PS-COOH NPs is striking. It appears that these cultures can be run almost indefinitely, but for our observation time, the particles appear to remain internalised, and persist unaffected. Furthermore, there is no evident biological impact on the cells during these longer times; this could suggest that polymer nanoparticle accumulation is almost indefinite, and that any biological impacts would be very subtle and require detailed biological analysis, possibly best accomplished in cultures of this type.

233

234 Conclusions

To date, most studies of long-term nanoparticle effects rely on *in vivo* animal models, which are costly and significantly different to human physiology. For materials that exhibit no chemical toxicity, long-term accumulation with few observable biological outcomes leads conventional toxicological studies to a 'dead end' in which, while there are no observable effects, the investigative tools are absent to explore novel concepts and fully determine the final outcomes.

In this work we have described a long-term 3D cell cluster culture platform produced by control 241 of the kinetics of cellular collision, division, and phenotypic evolution. When appropriate 242 cluster formation programs are chosen, dividing cells reach a quiescent state, coupled with the 243 244 establishment of an *in vivo*-like phenotype for long periods (potentially many months). These characteristics allow for longer term observations of nanoparticle cell interactions in a more 245 relevant environment, while preventing some of the drawbacks observed in standard monolayer 246 culture and other in vitro 3D culture models. Clusters formed with this technique are 247 reproducible, stable and viable for many weeks, and may be subjected to all the advanced tools 248 of modern molecular and cell biology. In addition, the cells comprising the clusters are 249

accessible to nanoparticles, allowing for conventional uptake studies in which all the cellsaccumulate and retain particles in much the same way as we believe tissue does.

252 The need for such tools is illustrated using two different formulations of SiO₂ nanoparticles

that degrade at different rates over several weeks depending on their synthesis method.

254 Significantly, (hydrocarbon based) polymeric nanoparticles are found to undergo no apparent

- 255 degradation over long time periods, nor do they have obvious biological impacts during this
- time. The availability of such cultures would now allow the whole range of modern biology to
- 257 be deployed in the question of whether there could be as yet undiscovered subtle effects of
- 258 nanomaterial accumulation over such very long periods of time. It is likely that question will
- attract considerable interest in the near future.
- 260

261 Materials and methods

262 Cell culture

A549 non-small lung carcinoma (ATCC[®] CCL-185[™]), HepG2 (ATCC[®] HB-8065[™]) and 263 HEK-293T (ATCC[®] CRL-11268[™]) cell lines were purchased from ATCC, and cultured in 264 MEM (Life Technologies) supplemented with 10% FBS (Life technologies) and 1% 265 penicillin/streptomycin (referred to hereafter as cMEM). Cells were grown at 37°C in a 266 humidified atmosphere of 5% CO₂ and sub-cultured at 70-80% confluence using trypsin 267 (0.25% in EDTA). Cells were screened monthly for mycoplasma contaminations using the 268 MycoAlertTM Mycoplasma Detection Kit, and all cultures were free of contamination for the 269 duration of experiments reported. 270

271

272 Nanoparticles

FluoSpheres[™] Carboxylate-Modified yellow-green fluorescent (505/515) polystyrene
nanoparticles (PS-COOH NPs; d: 100 nm) were used throughout the study (F8803; Thermo
Fisher Scientific). Characterization of the particles in PBS and cMEM was performed by
dynamic light scattering (DLS) measurement (Supp. Figure S28 and Table S4). Dye release
from the particles under different conditions was tested by SDS-PAGE (figure S30).

278 Silica (SiO₂) nanoparticles were prepared as described previously.^{50,51} Briefly, a fluorescein

- 279 isothiocyanate silane conjugate (FITC-APTMS) solution was prepared as follows: FITC (4
- mg) was dissolved in 2 ml of anhydrous ethanol, and 20 μ L of (3-Aminopropyl)trimethoxysilane (APTMS) was added. The mixture was incubated at room temperature while
- shaking for 4 hours, protected from light.⁵²
- 283 Preparation of the SiO_2 seeds:
- A solution composed of 21.6 mL ethanol and 0.24 ml tetraethyl orthosilicate (TEOS) was
- added quickly to a solution composed of 21.6 ml ethanol, 1.18 ml of NH₄OH solution (28-30
- 286 % w/w) and 114 µL of water. The mixture was left to react at room temperature for 2 hours.
- 287 Growing of the SiO_2 NP to 100 nm:

- A solution composed of 57.8 mL ethanol, 19.6 mL water, 1.12 ml NH4OH (28-30 % w/w), and
- 289 7 mL of the SiO₂ seed dispersion was prepared. Then 50 μ L of FITC-APTMS solution and 100
- μ L of TEOS were added. After 30 mins, another 50 μ L of the dye conjugate solution and 100
- μ L of TEOS was added. Then every 30 mins thereafter, 100 μ L of the dye conjugate solution
- and 200 μ L of TEOS was added until the particles reached a diameter of approximately 100 nm. Three hours after the last addition of TEOS, the NH₄OH was removed by evaporation
- under reduced pressure and the dispersion was centrifuged at 14,000 g during 10 min. The SiO₂
- 295 particles were washed 3 times with water by centrifugation.
- 296 Addition of the protective SiO_2 layer:
- 297 To make the SiO₂@SiO₂ particles, the SiO₂ nanoparticles were dispersed at 20 g/L and split
- into 2 mL centrifuge tubes (1.5 ml/tube) then 7 μ L of TEOS was added to each tube and the dispersion was heated while stirring at 90°C for 1 hour. Another 7 μ L was added and the particles were incubated again at 90°C for 3 hours. The particles were then washed with water 3 times by centrifugation.
- Size distribution of the SiO₂ nanoparticles was determined by DLS measurement after dispersion in water together with the zeta potential using a Zetasizer ZS series (Supp. Table S3), differential centrifugal sedimentation (DCS), considering a colloidal SiO₂ density of 2 g/cm^3 in a sucrose gradient (8-24% w/w in water), and transmission electron microscopy
- 306 (TEM) (Supp. Figure S25, Supp. Table S2).
- 307

308 Cell seeding and nanoparticle exposure

- A549 cells (2.5 x 10⁶) were seeded in 75 cm² flasks (in cMEM) and left to adhere for 24 hours. Prior to cell exposure, PS-COOH NPs were incubated at a final concentration of 0.1 mg/mL in cMEM at 37°C for 1 hour (to form the protein corona). Cells were exposed to this nanoparticle suspension for 4 hours at 37°C in a humidified atmosphere of 5% CO₂, while control cells
- suspension for 4 nours at 37 C in a numidified atmosphere of 5% CO₂, while control cells
- 313 received cMEM without nanoparticles. The suspension was then removed and the cells were
- 314 washed twice with cMEM and twice with PBS. After this washing step, cells were harvested 315 by trypsinisation and used for the following experiments.
- 315 by trypsinisation and used for the following experiments.
- 316 317

318 Cluster formation

319 Suspension media (SM) was prepared by diluting Happy Cell additive (Vale Life Sciences) from the stock solution of 4X to 1.7X with MEM supplemented with 1% 320 penicillin/streptomycin, and FBS was added to the solution to reach a final concentration of 321 10%. A549 cells were harvested from monolayer culture and resuspended in SM to a 322 concentration of 10⁵ cells/ml. 24 well plates were precoated with 400 µl of 1% agarose (Merck-323 Sigma) in MEM as described previously,⁵³ and then 700 µl of ASM was added on top. 1 ml of 324 SM containing the cells was then gently pipetted on top of this layer (this helps to avoid cell 325 sedimentation at the bottom of the well), resulting in a final cell number of 10⁵ cells/well. 326 Cluster formation was monitored during the following days by light microscopy, and a portion 327 of media was exchanged every other day. 328

329

330 Cluster harvesting

- 331 Cells in SM were harvested directly from the well and collected in falcon tubes. Inactivation
- 332 solution (Vale Life Sciences) was added to the cluster suspension to a final concentration of
- $333 \quad 60 \ \mu g/ml$, followed by 30 minutes incubation at $37^{\circ}C$ in a humidified atmosphere of 5% CO₂.
- After incubation, 7 ml of cMEM was added to the falcon tube to dilute the SM, and the clusters
- 335 were collected by centrifugation at 1,500 RPM for 3 minutes at room temperature. Supernatant

- 336 was removed, and the cells were resuspended in an appropriate buffer dependant on subsequent
- 337 processing.
- 338

339 Cluster disassembly and reseeding as monolayer culture

Clusters were harvested as described above every week and treated with Accutase® solution (Merck-Sigma) for 20 minutes at 37° C in a humidified atmosphere of 5% CO₂. The solution was pipetted thoroughly every 10 minutes to help the separation of the clusters into single cells.

- 343 Cells were then resuspended in fresh cMEM and seeded in 6 well plates, where they were
- harvested for analysis after 24 and 72 hours using trypsin.
- 345

346 Nanoparticle exposure to cell clusters

347 Prior to cell cluster exposure, the PS-COOH nanoparticles were incubated at a concentration of 1 mg/ml or 0.2 mg/ml in cMEM for 1 hour at 37°C to form the corona. Then 10% (volume) 348 of the SM containing clusters was removed from each well and substituted with the 349 nanoparticle suspension and mixed well (final concentration of the NPs in the well: 100 µg/ml 350 or 20 µg/ml). NP dispersion was checked by differential centrifugal sedimentation (DCS, Sup. 351 352 Figure S29). Cell clusters treated with cMEM with no particles were used as a control. After 4 hours of incubation, cell clusters were harvested from the SM as previously described and 353 354 washed twice with cMEM then twice with PBS to remove excess non-internalised particles. Clusters were then resuspended in fresh SM and cultured for extended periods (up to 2 weeks) 355 356 or used immediately.

357

358 Nanoparticle uptake assessment by flow cytometry

To dissociate the cell clusters for analysis by flow cytometry, they were harvested from SM 359 and washed once with PBS then disassembled using Accutase® solution (Merck-Sigma) as 360 previously described. Cells were then resuspended in 150 µl of cold PBS and immediately 361 analysed with an Accuri C6 (Becton Dickinson) with the following settings: flow rate 14 362 µl/min, factory laser and filter settings. To assess the cell uptake of nanoparticle, the fluorescent 363 signal of the internalised NPs was measured (excitation/emission 488/530 nm) for ≥10000 364 events collected in the population gated for single cells (gating strategy is presented in 365 Supplementary Figure S14). 366

367

368 Cell cycle analysis

369 The cell cycle of cells in monolayer or in clusters was assessed throughout the culture period using DNA and 5-ethynyl-2'-deoxyuridine (EdU) staining. Briefly, cells from monolayer 370 culture or suspension were treated for 1 hour with EdU, clusters were disassembled and then 371 372 fixed in 70% ethanol overnight at -20°C. Cells were stained using the Alexa 488 Click-It EdU 373 flow cytometry kit (Thermo Fisher) following manufacturer instructions. Before analysis, cells were resuspended in 1 µM Vybrant Dyecycle ruby stain (Thermo Fisher) in PBS and incubated 374 at 37°C for 30 minutes, then resuspended in PBS and analysed with an Accuri C6 (Becton 375 Dickinson) with the following settings: flow rate 14 µl/min, factory laser and filter settings. 376 For each sample, $\geq 10,000$ events in the population gated for single cells were collected (gating 377 strategy is presented in Supplementary Figure 14). 378

379

380 mRNA expression analysis

381 Cells were harvested from the SM or monolayer and washed once with PBS. Total RNA was

- extracted from cells using the Invitrap® Spin total RNA minikit (Invitek molecular) then
- 383 quantified using a Nanodrop 2000 (Thermo Fisher). RNA quality was checked using a

Bioanalyser (Agilent), with all samples having an RIN number of at least 8. cDNA was then obtained by reverse transcription using the High-Capacity cDNA Reverse Transcription Kit (Applied Biosystems) following manufacturer instructions. For qPCR analysis, SYBRTM Green PCR master mix (Thermo Fisher) was used together with the primers for the following genes of interest: Ki67, p27, E-CAD, MUC5AC, IgGFc, CTSB, CTSD, CTSL1, CTSS, CTSZ, TFEB; GAPDH was used as the housekeeping gene (Supplementary Table S5). Comparative Δ Ct method ($\Delta\Delta$ Ct) was used to calculate fold change in mRNA expression of targets.

391

392 MTS assay

For monolayer cells the MTS assay (Promega) was performed following manufacturer 393 instructions, using 1 minute incubation with 0.1% Triton X-100 (Merck-Sigma) for the positive 394 control for cytotoxicity. For cell clusters, a modification of the protocol was necessary. Briefly, 395 396 clusters were harvested from the SM as previously described, then resuspended in PBS and 397 divided into two equal volume samples. For both untreated and NP treated samples, one of the 398 two parts was treated with Accutase® as described and then resuspended in PBS. For the 399 untreated sample, this part was used to count the number of cells. Based on the number obtained, a volume of the untouched clusters was taken to make a solution with $5*10^4$ cells in 400 401 1.1 ml of MTS in cMEM. Same volume was used also for the NP treated sample, assuming that same number of cells was seeded in the beginning of the experiment. Then, 110 µl of MTS 402 solution (containing around $5*10^3$ cells in clusters for the untreated sample) were seeded in a 403 96 well plate in 3 technical replicates and incubated at 37°C and 5% CO₂ for one hour. Results 404 were then obtained by measuring absorbance at 490 nm using a plate reader (Varioskan Flash, 405 406 Thermofisher).

407

408 Live/Dead staining

409 Live-dead staining was performed on disassembled clusters. Briefly, 3 μ M DRAQ-7 dye 410 (BioStatus) was used to stain the cells was used to stain the cells suspended in PBS and 411 incubated on ice for 5 minutes, and the percentage of live and dead cells was recorded using 412 an accuri C6 (Becton Dickinson) with factory laser and filter settings. > 10,000 events were 413 recorded per sample (gating strategy is presented in Supplementary Figure S14).

414

415

416 Mass spectrometry analysis

417 Monolayer cells were washed 3 times with ice cold PBS and then harvested using a scraper. Clusters were harvested as described and washed 3 times with ice cold PBS. Following 418 centrifugation, cell pellets were resuspended in 8 M urea lysis buffer (8 M urea, 50 mM 419 NH₄HCO₃, and 1 mM EDTA, pH 8; reagents from Merck-Sigma) containing protease 420 421 inhibitors (cOmplete mini, Roche). Short sonication was used to break the cells and to fragment 422 the nuclear DNA, then the mixture was centrifuged at 20,000 x g for 15 minutes to pellet DNA and cell debris. The supernatant total protein was collected and quantified by BCA assay 423 (Thermo Fisher) and 40 µg was for preparation for mass spectrometry analysis. Briefly, the 424 total lysate was first reduced using DTT (10 mM), and alkylated by iodoacetamide (40 mM), 425 and then digested over night at room temperature using trypsin (enzyme to substrate ratio 1:50; 426 Thermo Fisher). Resulting peptides were purified using PierceTM C18 high capacity tips 427 (Thermo Fisher), and then dried and resuspended in 0.1% formic acid (Merck-Sigma). Analysis 428 429 was performed on technical triplicates by electrospray liquid chromatography mass spectrometry (LC-MS/MS) using an HPLC (Thermo Fisher) interfaced with an LTQ Orbitrap 430

- 431 (Thermo Fisher). MaxQuant and Perseus Software (Computational Systems Biochemistry,
 432 Max Planck institute, Martinsried) were used to analyse the data.
- 433

434 Cluster formation timelapse imaging

435 Cell clusters in SM were imaged directly in their plate using a Zeiss Axiovert 200M inverted

- 436 microscope with brightfield illumination and a 10x air objective. The cells were maintained at 437 37° C and 5% CO₂ for 24 hour timelapse (2 hour capture increment) and 48, 72, 96 and 120
- 437 37°C and 5% CO₂ for 24 hour timelapse (2 hour capture increment) and 48, 72, 96 and 120
 438 hours timelapse (3 hour capture increments), using the Zeiss software associated with the
 439 microscope. Further analysis of the images was performed using ImageJ software.
- 440

441 Spinning disc confocal Imaging

442 Cell clusters were imaged using 96-well glass bottom plates (Greinier Bio-one) on a Nikon 443 eclipse TI spinning disc confocal microscope. Clusters were fixed and permeabilsed prior to

- immunostaining with 4% paraformaldehyde and 0.1 Triton-X 100 (permeabilisation was not
- 445 needed for anti E-cadherin antibody). Antibodies used: Ki67 (Abcam ab92742), E-Cadherin
- (Abcam ab40772) and LAMP-1 (Abcam ab24170). As secondary antibody, an Alexa 546 was
 used in combination with every primary antibody (Thermo Fisher A11030 and Thermo Fisher
- 448 A11035). Images were analysed with Imaris imaging software (Bitplane) and ImageJ. For
- 449 wheat germ agglutinin (WGA) staining, the cell clusters were incubated with WGA 594 (5
- 450 μ g/ml) for 15 minutes at 37°C in a humidified atmosphere of 5% CO₂ and then washed with
- 451 PBS and fixed with 4% paraformaldehyde. DAPI ($2 \mu g/ml$) was used to counterstain the nuclei
- 452 of fixed cells prior to imaging. The Imaris imaging software was also used to render in 3D the
- 453 images in figure 1f and S4.
- 454

455 High content screening

- For cluster diameter assessment, cells were treated with WGA 594 and DAPI as previously described, and then imaged in 96 well glass bottom plates (Greiner Bio-one) using an Opera PhenixTM high content spinning disc microscope (Perkin Elmer). Long axis length distribution was assessed using the algorithm provided by the proprietary software (Harmony High-Content Imaging and Analysis software, Perkin Elmer). > 1,000 clusters were analysed for each timepoint.
- 462

463 Transmission electron microscopy

Cell clusters were washed with PBS and immediately fixed with 2.5% glutaraldehyde in 0.1 M 464 Sorensen phosphate buffer, rinsed with Sorensen phosphate buffer, and then post-fixed for 1 465 hour in 1% osmium tetroxide in deionised water. Cells were dehydrated in a graded ethanol 466 series (from 70% to 100%), followed by Acetone rinse. Samples were then immersed in an 467 468 Acetone/Epon (1:1 vol/vol) mixture for 1h before being transferred to pure Epon and embedded at 37°C for 2h. The final polymerization was carried out at 60°C for 24h. Ultrathin 469 sections of 80 nm, obtained with a diamond knife using an ultra-microtome Leica U6, were 470 supported on copper grids. Sections were stained with uranyl acetate and lead citrate before 471 472 being examined with an FEI TECNAI transmission electron microscope.

473

474 Statistical analysis

- 475 All data are shown as mean \pm SD as described in the figure captions. p < 0.05 was considered
- significant. The experiments were performed at least 3 times independently (with exception of
- 477 cell cycle analysis by flow cytometry and SiO_2 NPs degradation assessment, with 2
- independent replicates, cluster size distribution with one independent replicate per operator, 2

in total (see supp. Figures S31, 32 for independently replicated data from other operators). The number of independent replicates (N) performed for each experiment is indicated in each figure caption. Statistical analyses were performed using Prism 6.01 (GraphPad software). Student ttest and one-way ANOVA, the first two-sided with Welch correction and the latter with Turkey correction for multiple comparisons, were used as described in the figure captions. Statistical differences are defined as * p < 0.05; ** p < 0.01; *** p < 0.001.

485

486 **Conflict of interest:** Authors declare no conflict of interest.

487

Acknowledgments: The authors acknowledge Ms J Li, Ms W Zhang, and Mr X Yang for the 488 independent replications of some of the experiments. F.M. acknowledges the support of the 489 Irish Research Council Postgraduate fellowship (GOIPG/2015/2530). A.A. acknowledges the 490 491 Princess Nourah Bint Abdulrahman University Project Ref: IR10177, ID: 1056571209, M.M.C. acknowledges the support of the Irish Research Council Enterprise Partnership 492 Scheme (Postdoctoral) 2019 - EPSPD/2019/232. The authors acknowledge Dr. A. Blanco and 493 494 Dr. D. Scholtz from the Conway Institute of Biomolecular and Biomedical research centre flow cytometry and imaging core facilities in University College Dublin for their assistance, and Dr. 495 A. Davies from Vale Lifesciences for the support. 496 497

498 Supporting Information: All supporting information is available free of charge via the
499 Internet at http://pubs.acs.org.

500

501 **Author contributions:** F.M., M.M.C., and K.D. designed the experiments. F.M., A.A. and 502 V.A.G. performed the experiments and data analysis. L.A. synthesised and characterised the 503 two formulations of silica NP used in this study. F.M., Y.Y., M.M.C. and K.D. wrote and 504 revised the manuscript.

- **Data availability:** All relevant data during the study are available from the corresponding
- 507 authors upon request.

509	1.	Albanese, A., Tang, P. S. & Chan, W. C. W. The Effect of Nanoparticle Size, Shape,
510		and Surface Chemistry on Biological Systems. Annu. Rev. Biomed. Eng. 14, 1-16
511		(2012).
512	2.	Blanco, E., Shen, H. & Ferrari, M. Principles of Nanoparticle Design for Overcoming
513		Biological Barriers to Drug Delivery. Nat. Biotechnol. 33, 941-951 (2015).
514	3.	Pelaz, B. et al. Diverse Applications of Nanomedicine. ACS Nano 11, 2313-2381
515		(2017).
516	4.	Gong, N. et al. Carbon-Dot-Supported Atomically Dispersed Gold as a Mitochondrial
517		Oxidative Stress Amplifier for Cancer Treatment. Nat. Nanotechnol. 14, 379-387
518		(2019).
519	5.	Cedervall, T. et al. Understanding the Nanoparticle-Protein Corona Using Methods to
520		Quantify Exchange Rates and Affinities of Proteins for Nanoparticles. Proc. Natl. Acad.
521		Sci. 104, 2050–2055 (2007).
522	6.	Monopoli, M. P., Åberg, C., Salvati, A. & Dawson, K. A. Biomolecular Coronas Provide
523		the Biological Identity of Nanosized Materials. Nat. Nanotechnol. 7, 779–786 (2012).
524	7.	Tenzer, S. et al. Rapid Formation of Plasma Protein Corona Critically Affects
525		Nanoparticle Pathophysiology. Nat. Nanotechnol. 8, 772–781 (2013).
526	8.	Corbo, C. et al. The Impact of Nanoparticle Protein Corona on Cytotoxicity,
527		Immunotoxicity and Target Drug Delivery. Nanomedicine 11, 81–100 (2016).
528	9.	Saha, K. et al. Regulation of Macrophage Recognition through the Interplay of
529		Nanoparticle Surface Functionality and Protein Corona. ACS Nano 10, 4421-4430
530		(2016).
531	10.	Tsoi, K. M. et al. Mechanism of Hard-Nanomaterial Clearance by The Liver. Nat.
532		Mater. 15, 1212–1221 (2016).
533	11.	Lo Giudice, M. C., Herda, L. M., Polo, E. & Dawson, K. A. In Situ Characterization Of

- Nanoparticle Biomolecular Interactions in Complex Biological Media by Flow
 Cytometry. *Nat. Commun.* 7, 1–10 (2016).
- Bekdemir, A. & Stellacci, F. A Centrifugation-Based Physicochemical Characterization
 Method for the Interaction Between Proteins and Nanoparticles. *Nat. Commun.* 7, 1–8
 (2016).
- 539 13. Shapero, K. *et al.* Time and Space Resolved Uptake Study of Silica Nanoparticles by
 540 Human Cells. *Mol. Biosyst.* 7, 371–378 (2011).
- 541 14. Saha, K. *et al.* Surface Functionality of Nanoparticles Determines Cellular Uptake
 542 Mechanisms in Mammalian cells. *Small* 9, 300–305 (2013).
- Liu, M. *et al.* Real-Time Visualization of Clustering and Intracellular Transport of Gold
 Nanoparticles by Correlative Imaging. *Nat. Commun.* 8, 1–10 (2017).
- Khlebtsov, N. & Dykman, L. Biodistribution and Toxicity of Engineered Gold
 Nanoparticles: a Review of In Vitro and In Vivo Studies. *Chem. Soc. Rev.* 40, 1647–
 1671 (2011).
- Almeida, J. P. M., Figueroa, E. R. & Drezek, R. A. Gold Nanoparticle Mediated Cancer
 Immunotherapy. *Nanomedicine Nanotechnology, Biol. Med.* 10, 503–514 (2014).
- 18. Loos, C. *et al.* Functionalized Polystyrene Nanoparticles as a Platform for Studying BioNano Interactions. *Beilstein J. Nanotechnol.* 5, 2403–2412 (2014).
- Talamini, L. *et al.* Influence of Size and Shape on the Anatomical Distribution of
 Endotoxin-Free Gold Nanoparticles. *ACS Nano* 11, 5519–5529 (2017).
- Soenen, S. J. H. *et al.* Colloidal Gold Nanoparticles Induce Changes in Cellular and
 Subcellular Morphology. *ACS Nano* 11, 7807–7820 (2017).
- 556 21. Sandin, P. et al. The Biomolecular Corona is Retained During Nanoparticle Uptake and
- 557 Protects the Cells From the Damage Induced by Cationic Nanoparticles Until Degraded
- in the Lysosomes. *Nanomedicine Nanotechnology, Biol. Med.* 9, 1159–1168 (2013).

- De Matteis, V. *et al.* Negligible Particle-Specific Toxicity Mechanism of Silver
 Nanoparticles: the Role of Ag+ Ion Release in the Cytosol. *Nanomedicine Nanotechnology, Biol. Med.* 11, 731–739 (2015).
- Arami, H., Khandhar, A., Liggitt, D. & Krishnan, K. M. In Vivo Delivery,
 Pharmacokinetics, Biodistribution and Toxicity of Iron Oxide Nanoparticles. *Chem. Soc. Rev.* 44, 8576–8607 (2015).
- 565 24. Gao, C. *et al.* Y 2 O 3 Nanoparticles Caused Bone Tissue Damage by Breaking the
 566 Intracellular Phosphate Balance in Bone Marrow Stromal Cells. *ACS Nano* 13, 313–323
 567 (2019).
- 568 25. Hu, W. *et al.* Protein Corona-Mediated Mitigation of Cytotoxicity of Graphene Oxide.
 569 ACS Nano 5, 3693–3700 (2011).
- 570 26. Walkey, C. D. *et al.* Protein Corona Fingerprinting Predicts the Cellular Interaction of
 571 Gold And Silver Nanoparticles. *ACS Nano* 8, 2439–2455 (2014).
- 572 27. Sabella, S. *et al.* A General Mechanism for Intracellular Toxicity of Metal-Containing
 573 Nanoparticles. *Nanoscale* 6, 7052–7061 (2014).
- Jiang, Y. *et al.* The Interplay of Size and Surface Functionality on the Cellular Uptake
 of Sub-10 nm Gold Nanoparticles. *ACS Nano* 9, 9986–9993 (2015).
- 576 29. Corvaglia, S., Guarnieri, D. & Pompa, P. P. Boosting the Therapeutic Efficiency of
 577 Nanovectors: Exocytosis Engineering. *Nanoscale* 9, 3757–3765 (2017).
- 578 30. Kim, J. A., Aberg, C., Salvati, A. & Dawson, K. A. Role of Cell Cycle on the Cellular
- 579 Uptake and Dilution Of Nanoparticles In A Cell Population. *Nat. Nanotechnol.* 7, 62–
 580 68 (2012).
- 31. Rees, P. *et al.* Statistical Analysis of Nanoparticle Dosing in a Dynamic Cellular System. *Nat. Nanotechnol.* 6, 170–174 (2011).
- 583 32. Lee, J., Lilly, D., Doty, C., Podsiadlo, P. & Kotov, N. In Vitro Toxicity Testing of

- 584 Nanoparticles in 3D Cell Culture. *Small* **5**, 1213–1221 (2009).
- 585 33. Huang, K. *et al.* Size-Dependent Localization and Penetration of Ultrasmall Gold
 586 Nanoparticles in Cancer Cells, Multicellular Spheroids, and Tumors In Vivo. *ACS Nano*587 6, 4483–4493 (2012).
- 588 34. Huo, S. *et al.* Superior Penetration and Retention Behavior of 50 nm Gold Nanoparticles
 589 in Tumors. *Cancer Res.* 73, 319–330 (2013).
- 590 35. Mazuel, F. *et al.* Massive Intracellular Biodegradation of Iron Oxide Nanoparticles
 591 Evidenced Magnetically at Single-Endosome and Tissue Levels. *ACS Nano* 10, 7627–
 592 7638 (2016).
- 593 36. Eisenstein, M. Organoids: The Body Builders. Nat. Methods 15, 19–22 (2018).
- Montenegro, J.-M. *et al.* In Vivo Integrity of Polymer-Coated Gold Nanoparticles. *Nat. Nanotechnol.* 10, 619–623 (2015).
- 59638.Martinez, J. O. *et al.* Short And Long Term, In Vitro and In Vivo Correlations of Cellular
- and Tissue Responses to Mesoporous Silicon Nanovectors. *Small* **9**, 1722–1733 (2013).
- 598 39. Yeung, C.-Y. et al. In Vivo Toxicologic Study of Larger Silica Nanoparticles in Mice.

599 Int. J. Nanomedicine **12**, 3421–3432 (2017).

- 40. Lopez-Chaves, C. *et al.* Gold Nanoparticles: Distribution, Bioaccumulation and
 Toxicity. In Vitro and In Vivo Studies. *Nanomedicine Nanotechnology, Biol. Med.* 14,
 1–12 (2018).
- 41. Wyma, A. *et al.* Non-Newtonian Rheology in Suspension Cell Cultures Significantly
 Impacts Bioreactor Shear Stress Quantification. *Biotechnol. Bioeng.* 115, 2101–2113
 (2018).
- 42. Davies, A. Cell Suspension Medium and Cell Suspension Medium Additive for the
 Three Dimensional Growth of Cells. *Int. Pat.* 144372 Al, (2013).
- 608 43. Curcio, E. et al. Mass Transfer and Metabolic Reactions in Hepatocyte Spheroids

- 609 Cultured in Rotating Wall Gas-Permeable Membrane System. *Biomaterials* 28, 5487–
 610 5497 (2007).
- 44. Panieri, E. & Santoro, M. M. ROS Homeostasis and Metabolism: A Dangerous Liason
 in Cancer Cells. *Cell Death Dis.* 7, e2253 (2016).
- 613 45. Davison, C. A. *et al.* Antioxidant Enzymes Mediate Survival of Breast Cancer Cells
 614 Deprived of Extracellular Matrix. *Cancer Res.* 73, 3704–3715 (2013).
- 615 46. Gloushankova, N. A., Rubtsova, S. N. & Zhitnyak, I. Y. Cadherin-Mediated Cell-Cell
 616 Interactions in Normal and Cancer Cells. *Tissue Barriers* 5, 1–15 (2017).
- 47. Pampaloni, F., Reynaud, E. G. & Stelzer, E. H. K. The Third Dimension Bridges the
 Gap Between Cell Culture and Live Tissue. *Nat. Rev. Mol. Cell Biol.* 8, 839–845 (2007).
- 48. Thornell, I. M. *et al.* Gel-Forming Mucins Form Distinct Morphologic Structures in
 Airways. *Proc. Natl. Acad. Sci.* 114, 6842–6847 (2017).
- 49. Endl, E. *et al.* The Expression of Ki-67, MCM3, and P27 Defines Distinct Subsets of
 Proliferating, Resting, and Differentiated Cells. *J. Pathol.* 195, 457–462 (2001).
- 623 50. Reinhardt, N., Adumeau, L., Lambert, O., Ravaine, S. & Mornet, S. Quaternary
- 624 Ammonium Groups Exposed at the Surface of Silica Nanoparticles Suitable for DNA
- 625 Complexation in the Presence of Cationic Lipids. *J. Phys. Chem. B* **119**, 6401–6411 626 (2015).
- 627 51. Adumeau, L. *et al.* Impact of Surface Grafting Density of PEG Macromolecules on
 628 Dually Fluorescent Silica Nanoparticles Used for the In Vivo Imaging of Subcutaneous
 629 Tumors. *Biochim. Biophys. Acta Gen. Subj.* 1861, 1587–1596 (2017).
- Mahon, E., Hristov, D. R. & Dawson, K. A. Stabilising Fluorescent Silica Nanoparticles
 Against Dissolution Effects for Biological Studies. *Chem. Commun.* 48, 7970–7972
 (2012).
- 633 53. Friedrich, J., Seidel, C., Ebner, R. & Kunz-Schughart, L. A. Spheroid-Based Drug

634 Screen: Considerations and Practical Approach. *Nat. Protoc.* **4**, 309–324 (2009).





Figure 1: Formation and evolution of the cell clusters. a, Schematic illustration of the key
steps for cluster formation: an agar coating is first deposited to avoid cell attachment, and then

640 a layer of suspension media is added; cells are seeded on top of this layer to avoid excessive precipitation. **b**, Schematics of cluster formation and growth: when cells are suspended within 641 642 the suspension media, several stages of cluster growth occur. In the first hours most cells are singlets and can move and divide more often. Some cells eventually come in contact and 643 644 aggregate and so, in the second stage some clusters begin to form and become less mobile. In the third stage most clusters are fully formed, and further growth is limited. c, Gaussian fitting 645 646 of the distribution of cell cluster diameters determined by high content analysis microscopy show that growth is more rapid in the first 5 days, and then slows thereafter. This is supported 647 by d, extrapolation of the median and mean long axis length. e, Representative images of the 648 clusters at different time-points showing the initial growth and then a more stationary phase. 649 Nuclei are blue (DAPI) and plasma membrane is red (WGA547), scale bars = 50 μ m. f, 3D 650 reconstruction of clusters shows they are organised as an oblate shape and not spherical (scale 651 bars = $20 \mu m$). 652





Figure 2: mRNA and protein expression analysis of the clusters suggests a differentiation
of the cell phenotype towards a more *in vivo*-like representation. a, Increased E-cadherin
gene expression in clusters, together with confocal imaging (b and c) reveals a stronger
interaction between neighboring cells in suspension, compared to those grown in monolayer.
d, A significant upregulation of mucin 5AC and IgG Fc binding protein (e) expression suggests

an increase of mucus secretion from cells in the clusters (N = 4 mean \pm SD; * p < 0.05; ** p < 0.01; *** p < 0.001, calculated using one way ANOVA). This is supported by confocal image analysis of WGA stained monolayer cells (**f**) compared to 1 week old clusters (**g**) that show layers of mucus on the latter (scale bars = 20 µm). **h**, Representative TEM micrograph of a cell cluster after 3 weeks of culture shows very dense secretory granules in all the visible cells (circle and arrows; scale bar = 5 µm); **i**, mucus granules can be seen on the exterior of the cells (scale bar = 0.5 µm).





Figure 3: Cells cultured as clusters exit the cell cycle and are maintained in a quiescent 672 state. a, EdU vs dsDNA content scatter plots obtained by flow cytometry analysis show 673 changes in cell cycle phase distribution of monolayer and suspension cells after 24 hours and 674 2 weeks. b, The majority of cells are in the G0/1 phase after 1 week of suspension culture (N 675 = 2, mean \pm SD). **c**, Upregulation of p27^{Kip1} (a cell cycle inhibitor) together with the 676 downregulation of Ki67 (a proliferative cell marker) (d) suggests that the cells in clusters have 677 exited the cell cycle (mean \pm SD, N = 4; * p < 0.05; ** p < 0.01; *** p < 0.001, calculated 678 using one way ANOVA); e, Immunocytochemical localisation of Ki67 shows that while the 679

680 protein is present in the nucleus of all cells in monolayer, in clusters (f) it is mostly absent

681 (scale bars = $20 \ \mu m$).



684 Figure 4: Evaluation of polystyrene nanoparticle accumulation in clusters. a, Schematic illustration of nanoparticle treatment of cells in monolayer prior to cluster formation. b, The 685 686 intracellular PS-COOH NP fluorecscence intensity for monolayer cells decreased continually, while for the clusters, after an initial decrease of signal in first week, there was no significant 687 reduction thereafter (N = 3, mean \pm SD). **c-d**, Confocal imaging of monolayer and cell clusters 688 stained with WGA and DAPI 2 weeks from PS-COOH NP exposure shows that while few 689 690 particles are detected in the monolayer cells, many are still present within the cells in clusters. e, LAMP1 immunostaining confirms nanoparticle localisation in lysosomes after 2 weeks of 691 exposure in clusters. f, Schematic illustration of nanoparticle treatment of cells directly in 692 clusters. g, There is a significantly higher uptake in clusters compared to monolayer (N = 3 for 693 0.02 mg/mL, N = 4 for 0.1 mg/mL; mean \pm SD; *** p < 0.001, calculated using t-test). h, 694 Confocal imaging of disassembled clusters confirms a higher nanoparticle content in cells in 695 clusters compared to those in monolayer (i). j,l, maximum projection and (k,m) single Z-stack 696 imaging of clusters treated with nanoparticles at 0h chase time (**j-k**) and 24 hours chase time 697 (I-m) after treatment. Right after treatment many particles are still present on the surface of the 698 699 clusters, while at 24 hours all particles seem to be internalised (all scale bars in this figure = 20700 μm).



704 Figure 5: TEM micrographs of SiO₂ and SiO₂@SiO₂ NPs degradation in biological media

and A549 cell clusters. a, In cMEM both SiO₂ and SiO₂@SiO₂ nanoparticles show extensive

- degradation over a period of 2 weeks, while in artificial lysosomal fluid (ALF) no real effect
- is observed. **b**, In A549 cell clusters, while SiO₂@SiO₂ nanoparticles show only slight etching
- 708 on their surfaces after 4 weeks, for non-coated SiO₂ nanoparticles a greater degradative effect
- due to lysosomal action can be observed over the culture duration (scale bars = 100 nm).
- 710