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Effects of Unilateral Eccentric versus Concentric Training of Nonimmobilized Arm during Immobilization

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ABSTRACT

CHEN, T. C., S.-H. WU, H.-L. CHEN, W.-C. TSENG, K.-W. TSENG, H.-Y. KANG, and K. NOSAKA. Effects of Unilateral Eccentric versus Concentric Training of Nonimmobilized Arm during Immobilization. *Med. Sci. Sports Exerc.*, Vol. 55, No. 7, pp. 1195–1207, 2023. **Introduction:** The present study tested the hypothesis that eccentric training (ET) of nonimmobilized arm would attenuate negative effects of immobilization and provide greater protective effects against muscle damage induced by eccentric exercise after immobilization, when compared with concentric training (CT). **Methods:** Sedentary young men were placed to ET, CT, or control group ($n = 12$ per group), and their nondominant arms were immobilized for 3 wk. During the immobilization period, the ET and CT groups performed five sets of six dumbbell curl eccentric-only and concentric-only contractions, respectively, at 20%–80% of maximal voluntary isometric contraction (MVCiso) strength over six sessions. MVCiso torque, root-mean square (RMS) of electromyographic activity during MVCiso, and bicep brachii muscle cross-sectional area (CSA) were measured before and after immobilization for both arms. All participants performed 30 eccentric contractions of the elbow flexors (30EC) by the immobilized arm after the cast was removed. Several indirect muscle damage markers were measured before, immediately after, and for 5 d after 30EC. **Results:** ET increased MVCiso ($17\% \pm 7\%$), RMS ($24\% \pm 8\%$), and CSA ($9\% \pm 2\%$) greater ($P < 0.05$) than CT ($6\% \pm 4\%$, $9\% \pm 4\%$, $3\% \pm 2\%$) for the trained arm. The control group showed decreases in MVCiso ($-17\% \pm 2\%$), RMS ($-26\% \pm 6\%$), and CSA ($-12\% \pm 3\%$) for the immobilized arm, but these changes were attenuated greater ($P < 0.05$) by ET ($3\% \pm 3\%$, $-0.1\% \pm 2\%$, $0.1\% \pm 0.3\%$) than CT ($-4\% \pm 2\%$, $-4\% \pm 2\%$, $-1.3\% \pm 0.4\%$). Changes in all muscle damage markers after 30EC were smaller ($P < 0.05$) for the ET and CT than the control group, and ET than the CT group (e.g., peak plasma creatine kinase activity: ET, 860 ± 688 IU·L⁻¹; CT, 2390 ± 1104 IU·L⁻¹; control, 7819 ± 4011 IU·L⁻¹). **Conclusions:** These results showed that ET of the nonimmobilized arm was effective for eliminating the negative effects of immobilization and attenuating eccentric exercise–induced muscle damage after immobilization. **Key Words:** CROSS-EDUCATIONAL EFFECT, MUSCLE CROSS-SECTIONAL AREA, MUSCLE HARDNESS, DELAYED-ONSET MUSCLE SORENESS, MAXIMAL VOLUNTARY CONTRACTION, CREATINE KINASE

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Muscle disuse decreases muscle mass, muscle cross-sectional area (CSA), and force-generating capacity (1). Wall et al. (2) reported that immobilization by a full-leg cast for 5 d already reduced maximal voluntary isometric contraction (MVCiso) torque of the knee extensors ($-9.0\% \pm 2.3\%$) and quadriceps CSA ($-3.5\% \pm 0.5\%$). A longer period of immobilization (4–6 wk) could lead to greater decreases in muscle CSA for the elbow flexors (-11%) (3) and extensors (20% – 32%) (4), knee extensors (-16%), and soleus (-17%) as well as gastrocnemius (-26%) muscles (5).

It is well known that muscle strength gain conferred by a unilateral limb resistance training is transferred to a nontrained homologous muscle of the contralateral limb, which is referred to as the cross-education effect (6–8). A meta-analysis study by Munn et al. (8) showed that the magnitude of increase in muscle strength of the contralateral limb was 35% (95% confidence

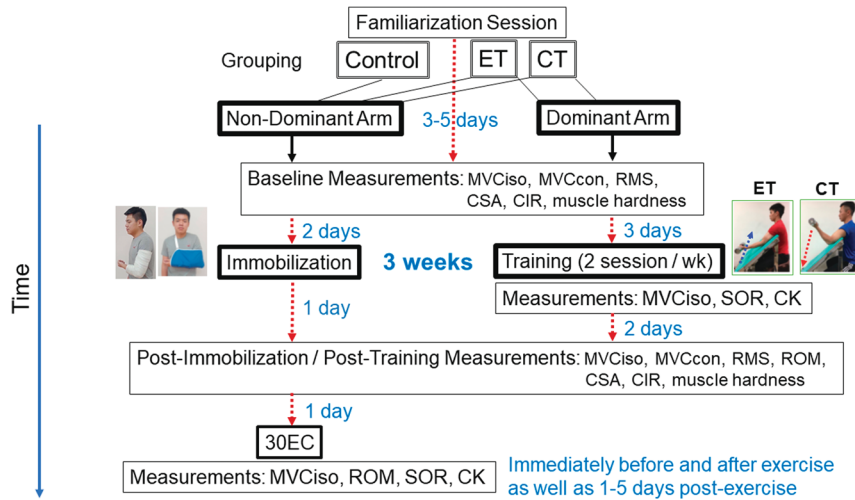


FIGURE 1—Experimental design and testing procedures of the study. The nondominant arms of the participants in the control, ET, and CT groups were immobilized for 3 wk, whereas the dominant arms of the participants of the ET and CT groups performed eccentric-only and concentric-only training of the elbow flexors twice a week during the 3-wk immobilization period. The nondominant arms performed 30 maximal eccentric contractions of the elbow flexors (30EC) after the immobilization. Multiple measurements were taken before and after immobilization from both arms, before and after each training session from the dominant arm, and before and after 30EC from the nondominant arm. CC, concentric contractions; CSA, biceps brachii cross-sectional area; MVC_{con}, maximal concentric contraction torque of the elbow flexors and extensors at 30°·s⁻¹; MVC_{iso}, maximal isometric contraction strength and torque at 90° of elbow flexion; RMS, root-mean square of surface electromyographic activity during MVC_{iso}; SOR, muscle soreness.

Immobilization

The nondominant arm was immobilized by a cast at the elbow joint of 90° flexion and secured in a sling with a mild shoulder internal rotation to unload the elbow flexor muscles (Fig. 1). This protocol was adapted and modified from previous studies that showed 13%–16% decreases in MVC_{iso} strength of the elbow flexors after a 2-wk immobilization of upper arm (17,18). The participants were instructed not to remove the sling except when changing their clothes, bathing, and sleeping.

Training during Immobilization

Each training session consisted of five sets of six eccentric-only or concentric-only contractions of the elbow flexors using a dumbbell. In the ET, each participant was instructed to lower a dumbbell from an elbow flexed (90°) to a fully extended position (0°) in 3 s, and the investigator removed the dumbbell at the extended position, and the arm was returned to the start position without a dumbbell. In the CT, each participant was instructed to lift a dumbbell from an elbow extended (≈5°) to a flexed position (90°) in 3 s. After each concentric contraction, the arm was returned to the start position without a dumbbell, and the investigator spotted a participant if he showed difficulty at long muscle lengths during the last training session in which a heavy weight was used. The interval was 15 s between contractions and 2 min between sets based on our previous study (9).

To determine the dumbbell weight for the progressive ET or CT, MVC_{iso} strength of the unilateral elbow flexors at 90° elbow flexion was measured by a loadcell (model DFG51; Omega Engineering, Stamford, CT) that was attached to a cuff surrounding the wrist of the exercise arm, according to our

previous study (9). It should be noted that MVC_{iso} strength is normally smaller than eccentric one-repetition maximum (1RM) strength but greater than concentric 1RM strength, and the MVC_{iso} strength at 90° elbow flexion is close to maximal eccentric and concentric strength at extended (<30° flexion) elbow joint angles (19). Because as few as two maximal eccentric contractions could attenuate the magnitude of muscle damage induced by the subsequent bout of maximal eccentric contractions of the same or opposite limb homologous muscle (20), the load for ET and CT was determined by the MVC_{iso} strength not by 1RM test. Each participant was seated on a custom-made preacher curl bench, placing the elbow joint angle at 90° and the shoulder joint angle at 45° flexion and 0° abduction. The participant was instructed to flex the elbow joint maximally for 3 s, and this was repeated three times with a 45-s rest between attempts. The highest value of the three peak values was used to determine the dumbbell weight (21).

The ET and CT protocols were modified from our previous study (9) showing that minimal muscle damage was induced in a 5-wk progressive eccentric resistance exercise training. The load for each exercise session in the present study was increased by 20%, 40%, 40%, 60%, 60%, and 80% of the MVC_{iso} strength that was reassessed at each week for both ET and CT (9). The training was performed twice a week with a 3-d rest between sessions. Changes in MVC_{iso} torque and muscle soreness of the trained arm, and plasma CK activity were measured before, and 1–2 or 1–3 d after each training session (Fig. 2).

Eccentric Exercise

All participants performed five sets of six eccentric contractions (30EC) of the elbow flexors of the immobilized arm with a dumbbell corresponding to the MVC_{iso} strength. Each

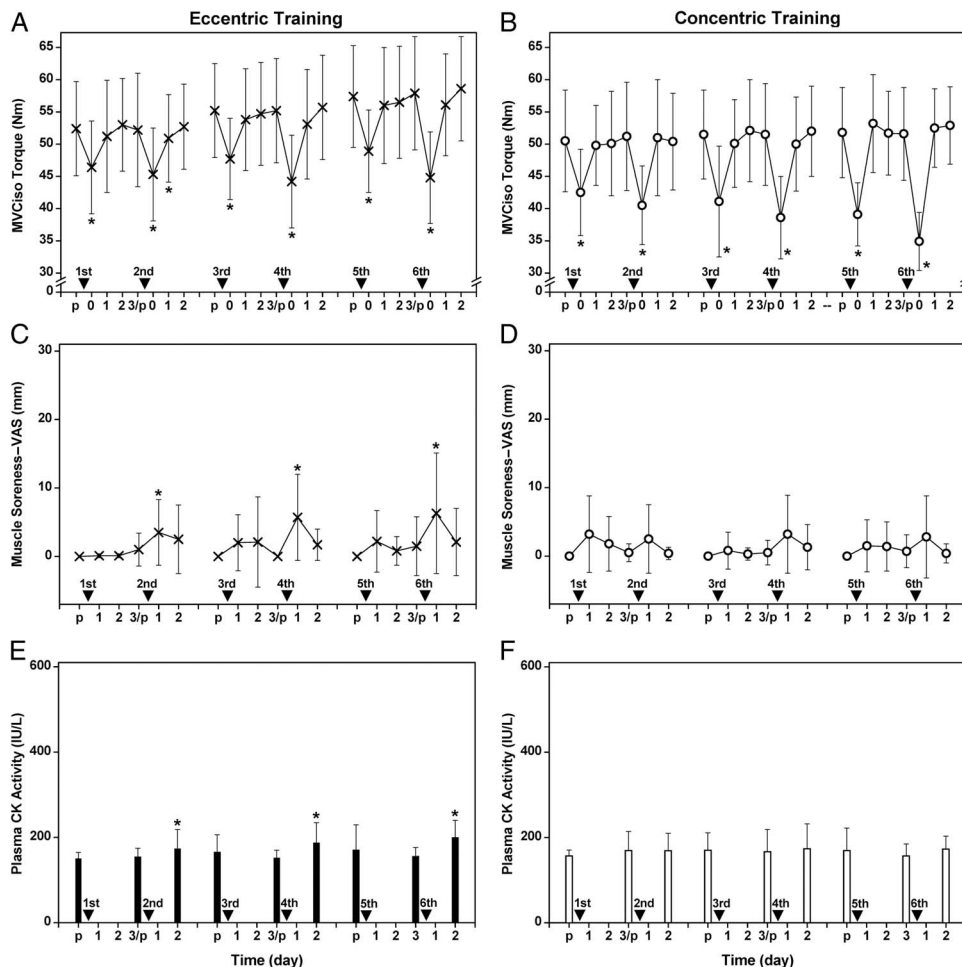


FIGURE 2—Changes (mean \pm SD) in MVCiso torque (A, B), muscle soreness assessed by a 100-mm visual analog scale (C, D), and plasma CK activity (E, F) activity before (p), immediately after (0), and 1–2 or 1 to 3 d after the first (20%), second (40%), third (40%), fourth (60%), fifth (60%), and sixth (80%) training sessions for the ET group (*left*) and CT group (*right*). *Significant difference ($P < 0.05$) from the pretraining value.

participant was instructed to lower a dumbbell from an elbow flexed (90°) to an elbow fully extended position (0°) in 3 s, and the investigator removed the dumbbell at the extended position, and the arm was returned to the start position without load. The eccentric contraction was repeated every 15 s, and a 2-min rest was inserted between sets (9).

Dependent Variables

The dependent variables consisted of MVCiso torque of the elbow flexors and MVCcon torque of the elbow flexors and extensors, root-mean square (RMS) during MVCiso, ROM, biceps brachii CSA by ultrasound extended-field-of-view (EFOV) imaging, CIR, muscle hardness, muscle soreness, and plasma CK activity. Among them, MVCiso torque, muscle soreness, and plasma CK activity were taken before, immediately after, and 1–2 or 1–3 d after each training session to monitor muscle damage for the ET and CT groups (Fig. 1). To assess the effects of immobilization on the immobilized and nonimmobilized arms, MVCiso and MVCcon torques, RMS, CSA, CIR, and muscle hardness were measured before and at 1 d after immobilization. To assess muscle damage after eccentric exercise for the immobilized arm, MVCiso torque, ROM, muscle soreness, and

plasma CK activity were assessed before, immediately after (only for MVCiso torque and ROM), and 1, 2, 3, 4, and 5 d after the exercise from the exercised arm.

MVCiso and MVCcon torques. The MVCiso and MVCcon torque measurements were the same as those of our previous study; thus, the details can be found in elsewhere (9,22). Briefly, the MVCiso torque was measured at 90° (1.57 rad) elbow flexion, where the full elbow extension angle was considered as 0° (0 rad) using a dynamometer (Biodex System S4; Biodex Medical Systems, Shirley, NY). The MVCcon torque was measured at the angular velocity of $30^\circ \cdot s^{-1}$ (0.52 rad $\cdot s^{-1}$) for the ROM of 120° (2.09 rad) for the elbow flexors (0° – 120°) and extensors (120° – 0°) for three continuous contractions for both directions by the isokinetic dynamometer, in the same position as that of the MVCiso torque measure. The MVCiso torque was measured first followed by the MVCcon torque measures with a 5-min rest between the MVCiso and MVCcon measures for each arm. Verbal encouragement was provided during the tests. The highest value of the three trials was used for further analysis of the MVCiso torque as well as the MVCcon torque of the elbow flexors (EF-MVCcon) and extensors (EE-MVCcon) (14).

Surface electromyography. Muscle activity was recorded using the Ultium EMG sensor system (Noraxon, INC, Scottsdale, AZ) with disposable Ag/AgCl pregelled electrodes during MVCiso measurements. The participants' skin was cleaned thoroughly and prepared before electrode placement. The surface electrodes were attached to the belly of the biceps brachii (2-cm center-to-center interelectrode distance). Raw EMG signals during the MVCiso measures were sampled with a frequency of 2000 Hz using a band-pass filter (10–500 Hz), and RMS was obtained for a 500-ms slot in the plateau MVCiso torque during the 3-s MVCiso (23). The average of peak RMS from three MVCiso trials on each time point was used for further analyses.

Range of motion. The ROM of the elbow joint was determined as the difference between the elbow joint angles of maximal voluntarily flexion and extension measured by a manual goniometer (9,24). Three measurements were taken for each angle, and the mean of the three measurements was used to calculate ROM (9,24).

Bicep brachii CSA. Using the EFOV method that was adapted from the previous study (25), biceps brachii was captured at 50% distal between the lateral epicondyle of the humerus and the acromial process of the shoulder. Each participant was lay supine in a comfortable position with arms fully resting on a massage bed. Pressure was applied minimally but consistently avoiding compression of the muscle, and transmission gel was applied to aid in acoustic coupling. EFOV scans were obtained using the same real-time B-mode ultrasound apparatus (Aloka Prosound $\alpha 6$ ultrasound system; Hitachi Co. Ltd., Tokyo, Japan) with a 7.5-MHz 4.0-cm probe (UST-5412) by moving the probe along the marked lines axially from the medial aspect to the lateral aspect of the upper arm in a continuous single view by the same investigator. Scanning velocity was controlled to allow clear EFOV images, and care was taken to avoid exerting too much pressure on the skin surface. Two scans were taken from each region, and the biceps brachii muscle was traced to calculate its CSA using a computer software program (ImageJ, version 0.0; National Institutes of Health, Bethesda, MD). Because some of the images did not include the whole area of brachialis clearly, only the biceps brachii CSA was obtained in the present study.

Upper arm circumference. While each participant was standing, relaxing, and letting the arm hang down by his side, the upper arm CIR was measured at the midportion of the upper arm, between the acromion process of the clavicle and the lateral epicondyle of the humerus, using a Gulick tape measure (Creative Health Products, Plymouth, MI). The measurements were taken three times by the same examiner, and the mean of the three measures was used for statistical analysis (9).

Muscle hardness. Muscle hardness was measured by a tissue hardness algometer (OE-220; Ito Co. Ltd., Tokyo, Japan) at the midportion of the biceps brachii (as the same site as that for the CSA measure) when each participant lay supine with the testing arm was fully extended and relaxed on a message

bed. Muscle hardness was measured three times at each time point, and the mean value of the three was calculated and used for further analysis (26).

Muscle soreness. Muscle soreness was quantified using a visual analog scale that had a 100-mm continuous line with “not sore at all” on one side (0 mm) and “very, very sore” on the other side (100 mm). The investigator asked the participant to rate his perceived soreness on the visual analog scale when the muscles were passively extended for the ROM (120°–0° of elbow flexion angles) measures (9,27).

Plasma CK activity. Approximately 5 mL of venous blood was withdrawn by a standard venipuncture technique from the cubital fossa region of the arm and centrifuged for 10-min to extract plasma, and plasma samples were stored at –80°C until analyses. Plasma CK activity was assayed spectrophotometrically by an automated clinical chemistry analyzer (Model 7080; Hitachi, Co. Ltd., Tokyo, Japan) using a commercially available test kit (Roche Diagnostics, Indianapolis, IN) (9,28).

Test-retest reliability of the measures. The test-retest reliability of the dependent variables except muscle hardness indicated by the coefficient of variation was shown to be smaller than 9.9% in the previous studies performed in the same laboratory and by the same investigators (9,25). Coefficient of variation of the muscle hardness measure that was assessed in our laboratory was 9.6%.

Cross-Education Effect

The cross-education effect ratio was calculated as the ratio between the trained and nontrained arms for the changes in MVCiso and MVCcon torques, RMS, CSA, CIR, and muscle hardness from pretraining to posttraining for each participant in the ET and CT groups by the following formula based on the previous study (29).

Cross-education effect ratio (%) = (change in the nontrained arm from pretraining to posttraining/change in the trained arm from pretraining to posttraining) \times 100.

In addition, the difference in each variable changes over the 3-wk immobilization period between the nonimmobilized and immobilized arms was examined to compare the magnitude of the cross-education effect among the three groups. The relationships between the changes in the variables in the nonimmobilized arm and those in the immobilized arm were also examined for the participants in each group.

Statistical Analyses

Shapiro–Wilk test was used to verify the normality assumption of the data, which showed that normality assumption was met for all variables in the present study. Baseline values of all dependent variables before the 3-wk immobilization were compared among the ET, CT, and control groups by a one-way ANOVA for the immobilized arm and nonimmobilized arm, separately. A mixed-design two-way ANOVA (group [3] \times time [2]) was used to compare the three groups for changes in each dependent variable before and after immobilization.

during MVCiso, biceps brachii CSA, and CIR for the trained arm, but a decrease in muscle hardness ($P = 0.001$) was found for the ET only. When comparing between the ET and CT groups, changes in all measures except for EE-MVCcon in the nonimmobilized (trained) arm were greater ($P \leq 0.001$) for the ET than CT group (interaction effect: MVCiso: $F_{1,22} = 21.3, \eta^2 = 0.492$; EF-MVCcon: $F_{1,22} = 182.3, \eta^2 = 0.892$; RMS: $F_{1,22} = 37.8, \eta^2 = 0.632$; CSA: $F_{1,22} = 75.9, \eta^2 = 0.775$; CIR: $F_{1,22} = 15.5, \eta^2 = 0.398$; hardness: $F_{1,22} = 28.8, \eta^2 = 0.567$).

Effects of training on the immobilized (nontrained) arm. A significant interaction effect among the three groups was evident for each variable (Table 1). The control group showed significant ($P < 0.05$) decreases in MVCiso, EF-MVCcon and EE-MVCcon torques, RMS of the biceps brachii during MVCiso, biceps brachii CSA, and CIR, and an increase in muscle hardness. Significant changes in these measures ($P < 0.05$) were also evident for the CT group, but the magnitude of the changes in MVCiso and EF-MVCcon torques, RMS, and muscle hardness was smaller ($P < 0.05$) when compared with the control group. In contrast, the ET group showed significant ($P < 0.05$) increases in MVCiso and EF-MVCcon torques, and RMS during MVCiso; a decrease in muscle hardness; and no significant changes in CSA and CIR. When comparing with the control group, changes in all variables were significantly smaller ($P < 0.001$) for the ET group (interaction effect; MVCiso: $F_{1,22} = 253.4, \eta^2 = 0.920$; EF-MVCcon:

$F_{1,22} = 111.0, \eta^2 = 0.835$; EE-MVCcon: $F_{1,22} = 30.1, \eta^2 = 0.578$; RMS: $F_{1,22} = 71.1, \eta^2 = 0.764$; CSA: $F_{1,22} = 113.1, \eta^2 = 0.837$; CIR: $F_{1,22} = 183.3, \eta^2 = 0.893$; hardness: $F_{1,22} = 169.0, \eta^2 = 0.885$) and CT group (interaction effect; MVCiso: $F_{1,22} = 96.3, \eta^2 = 0.814$; EF-MVCcon: $F_{1,22} = 22.4, \eta^2 = 0.504$; EE-MVCcon: $F_{1,22} = 67.7, \eta^2 = 0.755$; RMS: $F_{1,22} = 27.8, \eta^2 = 0.558$; CSA: $F_{1,22} = 58.8, \eta^2 = 0.728$; CIR: $F_{1,22} = 60.0, \eta^2 = 0.732$; hardness: $F_{1,22} = 61.5, \eta^2 = 0.737$). When comparing the ET and CT groups, the changes were significantly smaller ($P < 0.001$) for the ET than CT group (interaction effect; MVCiso: $F_{1,22} = 106.6, \eta^2 = 0.829$; EF-MVCcon: $F_{1,22} = 19.0, \eta^2 = 0.464$; EE-MVCcon: $F_{1,22} = 116.3, \eta^2 = 0.841$; RMS: $F_{1,22} = 74.1, \eta^2 = 0.771$; CSA: $F_{1,22} = 37.1, \eta^2 = 0.628$; CIR: $F_{1,22} = 98.7, \eta^2 = 0.818$; hardness: $F_{1,22} = 144.0, \eta^2 = 0.867$).

Cross-education effects. The cross-education effect ratio was significant ($P \leq 0.001$) for MVCiso torque ($21.7\% \pm 8.3\%$), EF-MVCcon torque ($36.8\% \pm 20.4\%$), RMS ($43.5\% \pm 12.7\%$), and CIR ($6.1\% \pm 11.8\%$) in the ET group only. As shown in Figure 3, a significant ($P < 0.02$) correlation between the nonimmobilized (trained) and immobilized arms was found in the ET and CT groups for the changes in MVCiso (ET: $r = 0.804$, CT: $r = 0.625$) and RMS (ET: $r = 0.892$, CT: $r = 0.840$) only.

Changes in muscle damage markers after 30EC. All groups showed significant ($P < 0.05$) changes in MVCiso

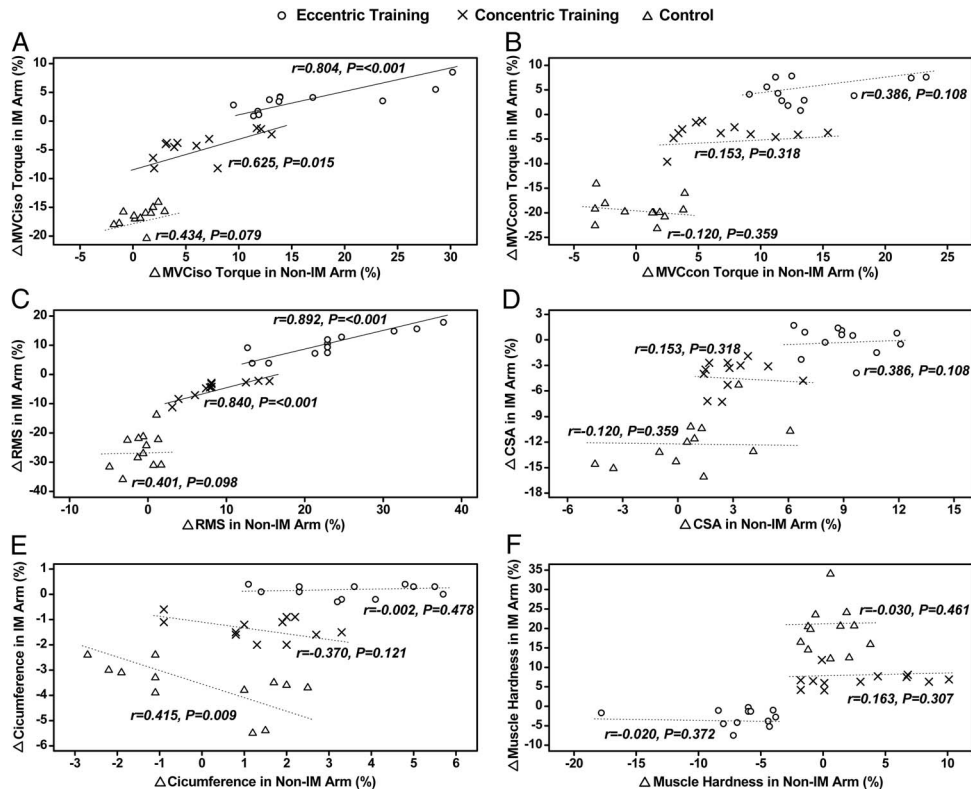


FIGURE 3—Correlations between the nonimmobilized (Non-IM) and immobilized (IM) arms for the magnitude of changes in maximal voluntary isometric (MVCiso; A) and concentric contraction torque of the elbow flexors (MVCon; B), RMS of surface electromyographic activity during MVCiso (RMS; C), biceps brachii cross-sectional area (CSA; D), CIR (E), and muscle hardness (F) over 3-wk immobilization period for the ET (shown by x), CT (shown by o), and control (shown by Δ) group ($n = 12$ per group), respectively. A solid line represents a significant ($P < 0.05$) correlation, and a dotted line represents a nonsignificant ($P > 0.05$) correlation.

torque, ROM, muscle soreness, and plasma CK activity after 30EC performed by the immobilized arm (Fig. 4). A significant interaction effect ($P < 0.05$) was evident for changes in MVCiso torque ($F_{12,198} = 14.2$, $\eta^2 = 0.462$), ROM ($F_{12,198} = 28.7$, $\eta^2 = 0.635$), muscle soreness ($F_{10,165} = 10.4$, $\eta^2 = 0.387$), and plasma CK activity ($F_{10,165} = 28.5$, $\eta^2 = 0.633$) over time among the three groups. When compared with the control group, the changes were significantly smaller for the ET group (interaction effect; MVCiso: $F_{6,132} = 27.0$, $P < 0.001$, $\eta^2 = 0.551$; ROM: $F_{6,132} = 66.4$, $P < 0.001$, $\eta^2 = 0.751$; muscle soreness: $F_{5,110} = 18.1$, $P < 0.001$, $\eta^2 = 0.451$; plasma CK activity: $F_{5,110} = 35.5$, $P < 0.001$, $\eta^2 = 0.618$) and the CT group (MVCiso: $F_{6,132} = 8.0$, $P < 0.001$, $\eta^2 = 0.266$; ROM: $F_{6,132} = 5.4$, $P < 0.001$, $\eta^2 = 0.198$; muscle soreness: $F_{5,110} = 3.8$, $P = 0.003$, $\eta^2 = 0.147$; CK: $F_{5,110} = 23.6$, $P < 0.001$, $\eta^2 = 0.517$). The changes in the ET group were significantly ($P < 0.001$) smaller than those of the CT group for all variables (MVCiso: $F_{6,132} = 7.1$, $\eta^2 = 0.244$; ROM: $F_{6,132} = 26.4$, $\eta^2 = 0.546$; muscle soreness: $F_{5,110} = 9.2$, $\eta^2 = 0.296$; CK: $F_{5,110} = 11.2$, $\eta^2 = 0.338$).

Figure 5 compares the magnitude of the protective effect for each variable and the average of the four variables (MVCiso, ROM, muscle soreness, and plasma CK activity) between the ET and CT groups. The average protective effect from the values of the four variables was greater ($F_{1,5} = 109.7$, $P < 0.001$, $\eta^2 = 0.956$) for the ET group (83.3% \pm 13.9%) than the CT group (43.3% \pm 17.4%).

DISCUSSION

The results seem to support the hypotheses that 1) ET would attenuate decreases in neuromuscular function and CSA of the immobilized arm greater than CT, and 2) ET would provide greater protective effects against muscle damage induced by maximal eccentric exercise after immobilization than CT. In the sections hereinafter, hypotheses 1 and 2 are discussed, and practical applications and future research directions are provided.

Effects of ET versus CT on trained and immobilized arms. The CT decreased MVCiso torque only at immediately after exercise, and no muscle soreness was developed after CT (Fig. 2). This suggests that no muscle damage was induced by CT, which was in line with the finding of previous studies (9,31). In ET, decreases in MVCiso torque lasted for 2 d after exercise, and increases in muscle soreness and plasma CK activity were observed after the second, fourth, and sixth training sessions. These indicate that muscle damage was induced at the higher-intensity (>40%) ET, but the magnitude of muscle damage was minor. Tseng et al. (9) also reported that the magnitude of muscle damage induced by eccentric exercise of the elbow flexors was minor, when the intensity of eccentric contractions was progressively increased from 10% to 100% of preexercise MVCiso level in a 5-wk ET.

No significant changes in any of the variables for the nonimmobilized arm were found for the control group, but the ET and CT groups showed significant changes in all variables after the 3-wk training for the nonimmobilized trained arm (Table 1). The normalized changes in all variables from

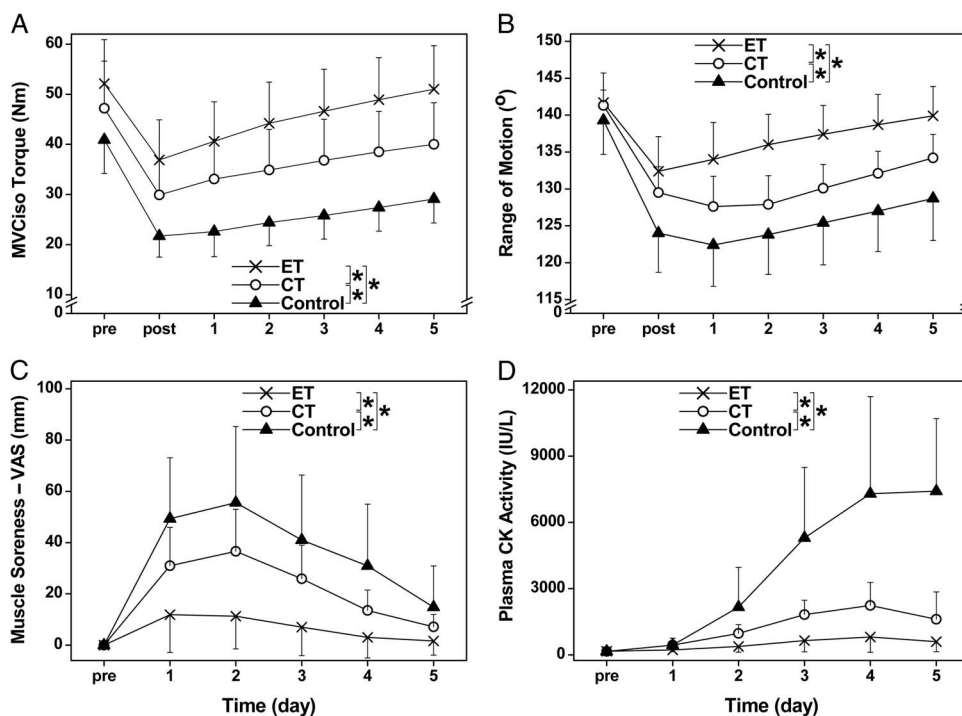


FIGURE 4—Changes (mean \pm SD) in MVCiso torque (A), ROM (B), and changes in muscle soreness by 100-mm visual analog scale (C), and plasma CK activity (D) from the baseline (pre) at immediately (0), and 1, 2, 3, 4, and 5 d after maximal eccentric exercise of the elbow flexors for the control, ET, and CT groups. *Significant ($P < 0.05$) interaction effect by mixed-design two-way ANOVA for the corresponding two groups.

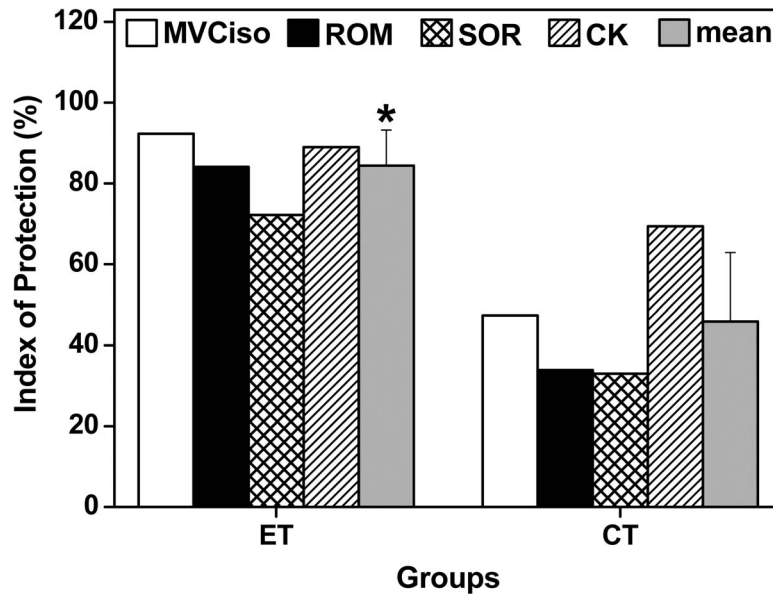


FIGURE 5—Index of protection for MVCiso torque of the elbow flexors, ROM, muscle soreness (SOR), and plasma CK activity, and the average and SD of the six variables (mean) for the ET and CT groups. The index was based on the comparison to the changes after the bout of the control group, which was calculated by the formula: $[\text{Change in the control condition} - \text{Change in ET or CT group}] / [\text{Change in the control group}] \times 100\%$. The “Change” in the formula refers to the magnitude of the change from the baseline at 5 d after exercise for MVCiso and ROM, and maximal change from the baseline for SOR and CK. *Significant ($P < 0.05$) difference from the CT group by a *t*-test.

baseline were greater for the ET than CT group. These results were consistent with the findings of previous training studies in which eccentric-only and concentric-only training were compared (9,29,32,33). These suggest that eccentric-only resistance training produces greater neuromuscular adaptations than concentric-only resistance training.

Regarding the changes in the variables of the immobilized arm, the control group showed decreases in MVCiso (−17%), EF-MVCcon (−19%), EE-MVCcon torque (−12%), RMS (−26%), CSA (−12%), and CIR (−4%) and an increase in muscle hardness (20%). Some of these changes were similar to those reported after a 3-wk sling immobilization ($15 \text{ h} \cdot \text{d}^{-1}$) of the elbow flexors (1RM strength: −20%, muscle thickness: −6%) in a previous study (34). Thus, it seems that the magnitude of decreases in muscle strength and size in the control group was comparable to that normally induced by immobilization of the elbow flexors for the duration. These changes were smaller for the CT group, and importantly, the ET group showed increases in MVCiso (4%) and EF-MVCcon torque (5%) without changes in CSA (−0.1%) and CIR (0.1%), and a decrease in muscle hardness (−3%) (Table 1). Valdes et al. (11) reported that a 4-wk sling immobilization ($8 \text{ h} \cdot \text{d}^{-1}$) of the elbow flexors decreased CIR by 5%, MVCiso torque by 22% and RMS during MVCiso by 35%, but these decreases were significantly attenuated by concentric–eccentric coupled resistance training (no decrease in MVCiso torque, 5.9% decrease in RMS, 2.1% decrease in arm circumference) that were performed three times a week by the nonimmobilized arm. Interestingly, they reported that MVCiso torque and RMS of the elbow flexors increased 12% and 17.5%, respectively in the immobilized arm when the nonimmobilized arm performed

eccentric-only resistance training with a heavier dumbbell (11). The present study also found an increase in MVCiso torque and RMS after eccentric-only training for the non-trained (immobilization) arm, although the magnitude of the increase was smaller than that reported in the study by Valdes et al. (11). They speculated that eccentric-only training modulated the corticospinal and intracortical inhibition to a greater extent than the coupled concentric-ET. It may be that the 1RM tests performed by the trained arm during the ET and CT at before the first, third and fifth training sessions (9 tests in total) contributed to the cross-over effect (35,36). However, it is important to note that the same number of 1RM tests was performed by the ET and CT groups, thus the difference in the cross-education effect between the two groups cannot be explained by the 1RM tests.

It should be noted that no significant correlation between the nonimmobilized and immobilized arms was evident for the changes in the variables for the control group (Fig. 3). This may suggest that the immobilized arm was not influenced by the nonimmobilized arm without exercise training. A significant correlation between the trained and immobilized arms of the participants in the ET and CT groups was evident for the changes in MVCiso (ET: $r = 0.804$, CT: $r = 0.625$) and RMS (ET: $r = 0.892$, CT: $r = 0.840$) (Fig. 3). It appears that the greater the training effects, the greater the cross-education effect at least for MVCiso torque and its related variable (i.e., RMS during MVCiso). It is interesting that such a relationship was not observed for MVCcon, biceps brachii CSA, CIR and muscle hardness. This may be due to the small sample size, but it is puzzling how exactly the trained arm influenced the immobilized arm for some of the variables only.

resistance exercise (six sessions) of the contralateral arm. The magnitude of the contralateral protective effect conferred by the ET (average of MVC_{iso}, ROM, and muscle soreness; 83%) in the present study (Fig. 4) seems to be greater than that of the contralateral repeated bout effect reported in the previous study (14) reporting that the effect was 69% for 1-d and 52% for 7-d interval between bouts.

Hyldahl et al. (41) have documented that the repeated bout effect is induced by a combination of neural adaptations, muscle–tendon complex behavior changes, extracellular matrix structural remodeling, and modified inflammatory responses. It seems likely that the contralateral protective effect is related more to neural and modified inflammation adaptations, although adaptations at muscle–tendon complex and extracellular matrix should be not ruled out. It may be that the underlying mechanisms of the contralateral protective effect are somewhat similar to those of the cross-education effect in which a resistance training of one limb increases muscle strength of the contralateral limb (9–11). As described previously, the sparing effects of cross-education may be potentially elicited to the muscle damage protective effect. It is possible that adaptations at the cortical and spinal levels were involved in the contralateral muscle damage protective effect conferred by the ET and CT. Kidgell et al. (33) showed that the extent of the cross-education effect on MVC_{iso} of the wrist flexors was significantly greater after ET (+47%) than CT (+28%) performed three times a week for 4 wk. They also showed that ET modulated corticospinal excitability and inhibition of the untrained limb to a greater extent than CT. It seems possible that the effects of eccentric contractions performed by the nonimmobilized arm were transferred to the contralateral immobilized arm greater. In a review article, Hendy and Lamon (40) proposed that functional reorganization of the motor cortex would facilitate the effects of cross-education, and cross-activation of the “untrained” motor cortex (ipsilateral to the trained limb) by increased neural drive from the “untrained” motor cortex contributes to the cross-education effect. These may be associated with the contralateral muscle damage protective effect observed in the previous study (9).

As for the inflammation or systemic factors, it has been documented that modified inflammatory or systemic factors play a role in the contralateral repeated bout effect (41,42). Xin et al. (42) reported that an increase in inflammatory-related transcription factor nuclear factor κ -light-chain-enhancer of activated B cells (NF- κ B) after the second bout was significantly attenuated not only in the vastus lateralis that was used in the maximal eccentric contractions of the ipsilateral knee extensors (123% \pm 3%; relative to the control leg without exercise) but also in the opposite leg that was not used in the exercise (109% \pm 3%). Because the NF- κ B is an effector of an upstream mechanistic pathway, it could be transferred to the nonexercising muscles (42). Thus, this might be associated with the contralateral muscle damage protective effect found in the present study. As shown in Table 1, the ET reduced muscle hardness (muscle became more compliant) not only

in the trained arm but also in the immobilized arm. It is not known how this happened, but it has been shown that compliant muscles are less susceptible to eccentric exercise–induced muscle damage (43,44). Thus, it may be that the immobilized arm of the ET group was more resilient to mechanical strain in 30EC. More studies are warranted to investigate the mechanisms underpinning the muscle damage protection including the contralateral one.

Limitations of the present study. The current study has several limitations. First, only young sedentary men were used as participants; thus, it is not known whether other populations such as women, elderly and fragile individuals, or people with chronic diseases respond similarly. Second, the current study did not monitor physical activity of the immobilized arm during the experiment. Third, the present study did not include eccentric strength measures, because eccentric strength measures would affect the adaptations (12,32). However, it is interesting to investigate how eccentric strength changes with the ET, CT, and control condition in a future study. Fourth, EMG was only taken from the biceps brachii during the MVC_{iso} torque measures, and EMG activity was not normalized in the present study. Fifth, the results of the present study could not be generalized to other muscles such as leg muscles (e.g., knee extensors and flexors) as mentioned previously. Fifthly, because of the relatively small sample size for the correlation analyses ($n = 12$ per group), the interpretation of the correlation results needs to be confirmed in a study with a larger sample size. Lastly, the current study was rather descriptive, and a mechanistic approach (e.g., biopsies, measures of protein regulation) to examine the possible mechanisms underpinning the effects was not investigated.

Practical significance and future research directions. The findings of the current study provide some useful information for prevention of muscle strength loss and atrophy by immobilization, and attenuation of muscle damage by resistance exercise after immobilization. To minimize the negative effects of immobilization, resistance training using eccentric contractions of the nonimmobilized arm can be recommended. It is important to investigate further if the findings of the present study are replicated for other muscles such as elbow extensors, knee extensors, and plantar flexors.

It is necessary to investigate whether eccentric resistance training of nonimmobilized muscles is effective for attenuating or maintaining the negative effects of immobilization in real injuries such as ligament sprains or tears, bone fracture, and postsurgery (e.g., joint replacement, anterior cruciate ligament) that accompany inflammation. Previous studies (45–50) have shown that the cross-education effects are still observed in musculoskeletal injuries when a nonaffected limb receives a resistance training, but ET was not used in these studies. It is also interesting to apply the contralateral eccentric resistance training to a less impaired limb for patients with stroke, as two studies showed that resistance exercise training of a less impaired limb provides positive effects on an impaired limb

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