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1 **Evaluation of intraperitoneal [<sup>18</sup>F]-FDOPA administration for micro-PET imaging in**  
2 **mice and assessment of the effect of sub-chronic ketamine dosing on dopamine**  
3 **synthesis capacity**

4

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21

22 **Abstract**

23 Positron emission tomography (PET) using the radiotracer [<sup>18</sup>F]-FDOPA provides a tool for studying brain  
24 dopamine synthesis capacity in animals and humans. We have previously standardised a micro-PET  
25 methodology in mice by intravenously administering [<sup>18</sup>F]-FDOPA via jugular vein cannulation, and  
26 assessment of striatal dopamine synthesis capacity, indexed as the influx rate constant  $K_i^{Mod}$  of [<sup>18</sup>F]-FDOPA,  
27 using extended graphical Patlak analysis with the cerebellum as a reference region. This enables a direct  
28 comparison between preclinical and clinical output values. However, chronic intravenous catheters are  
29 technically difficult to maintain for longitudinal studies. Hence, in this study, intraperitoneal administration  
30 of [<sup>18</sup>F]-FDOPA was evaluated as a less invasive alternative that facilitates longitudinal imaging. Our  
31 experiments comprised the following assessments: (i) comparison of [<sup>18</sup>F]-FDOPA uptake between  
32 intravenous and intraperitoneal radiotracer administration and optimisation of the time window used for  
33 extended Patlak analysis, (ii) comparison of  $K_i^{Mod}$  in a within-subject design of both administration routes, (iii)  
34 test-retest evaluation of  $K_i^{Mod}$  in a within-subject design of intraperitoneal radiotracer administration, and  
35 (iv) validation of  $K_i^{Mod}$  estimates by comparing the two administration routes in a mouse model of  
36 hyperdopaminergia induced by sub-chronic ketamine.

37 Our results demonstrate that intraperitoneal [<sup>18</sup>F]-FDOPA administration resulted in good brain uptake, with  
38 no significant effect of administration route on  $K_i^{Mod}$  estimates (intraperitoneal:  $0.024 \pm 0.0047 \text{ min}^{-1}$ ,  
39 intravenous:  $0.022 \pm 0.0041 \text{ min}^{-1}$ ,  $p=0.42$ ) and similar coefficient of variation (intraperitoneal: 19.6%;  
40 intravenous: 18.4%). The technique had a moderate test-retest validity (intraclass correlation coefficient,  
41 ICC=0.52, N=6), and thus supports longitudinal studies. Following sub-chronic ketamine administration,  
42 elevated  $K_i^{Mod}$  as compared to control condition was measured with a large effect size for both methods  
43 (intraperitoneal: Cohen's  $d=1.3$ ; intravenous: Cohen's  $d=0.9$ ), providing further evidence that ketamine has  
44 lasting effects on the dopamine system, which could contribute to its therapeutic actions and/or abuse  
45 liability.

46

## 47 Introduction

48 The radiotracer [<sup>18</sup>F]-fluoro-3,4-dihydroxyphenyl-L-alanine ([<sup>18</sup>F]-FDOPA) has been used to non-invasively  
49 study presynaptic dopamine synthesis capacity in the human brain using positron imaging tomography (PET)  
50 for nearly four decades [1-4]. [<sup>18</sup>F]-FDOPA PET imaging has been instrumental to demonstrate altered  
51 dopamine function due to stress, pharmacological challenges, and the pathology of neurodegenerative  
52 disorders and psychiatric illness [3, 5-11]. In schizophrenia, specifically, [<sup>18</sup>F]-FDOPA PET imaging has revealed  
53 elevated dopamine synthesis capacity in the striatum of patients as well as those at high risk or in the  
54 prodromal phase of schizophrenia [12-17]. Conversely, patients with neurodegenerative disorders like  
55 Parkinson's disease show decreased uptake in the same region [18, 19]. Thus, [<sup>18</sup>F]-FDOPA PET imaging is a  
56 critical tool in medical research for diagnostics and monitoring disease progression, as well as for elucidating  
57 underlying disease pathology and assessing effectiveness of existing and novel pharmacological treatments.

58 In more recent years, the development of micro-PET technology [20] has enabled the study of small animal  
59 models of human disease, allowing for translational investigation of underlying pathology and supporting the  
60 development of novel therapies. Mice and rats in particular offer the advantage of being experimentally  
61 tractable models, including the generation of phenotypes by pharmacological treatment, genetic models  
62 using protein knockout or overexpression, and functional manipulation using optogenetic or chemo-genetic  
63 regulation [21-23]. Work from our group recently showed that sub-chronic ketamine treatment in mice  
64 resulted in elevated striatal dopamine synthesis capacity, resembling the dopaminergic alteration seen in  
65 patients with schizophrenia, and demonstrated that this measure could be reduced using pharmacological  
66 treatment [24].

67 In mice, radiotracers for PET imaging are routinely administered intravenously (i.v.), particularly via the  
68 superficial tail vein. However, repeated administration can lead to injury and, due the small bore of this vein,  
69 the injectable volume is limited, while partial paravenous injection is a risk that can lead to inadequate  
70 radiotracer delivery. Jugular vein cannulation, which enables fast delivery to the brain, is a challenging and  
71 invasive procedure in mice which is normally a terminal procedure as recovery after extended anaesthesia is  
72 challenging, thus preventing longitudinal assessments. In the case of longitudinal studies, chronic  
73 intravenous catheters are technically difficult to maintain and can be stressful to mice. L-3,4-  
74 dihydroxyphenylalanine (L-DOPA) is absorbed in the rat peritoneum with less interindividual variability than  
75 oral dosing [25]. However, it is not known if this is the case in mice, where difference in size and metabolism  
76 may affect radiotracer uptake in the brain.

77 In the current study, we investigated intraperitoneal (i.p.) [<sup>18</sup>F]-FDOPA administration to evaluate dopamine  
78 synthesis capacity, expressed as rate constant  $K_i^{mod}$ , in mice in four steps. In experiment 1 we compared [<sup>18</sup>F]-  
79 FDOPA uptake between i.v. and i.p. radiotracer administration and optimised the time window used for  
80 estimation of  $K_i^{mod}$ . Experiment 2 compared  $K_i^{mod}$  in a within-subject design between i.v. and i.p. routes of  
81 administration of the radiotracer. Experiment 3 evaluated test-retest correlation of  $K_i^{mod}$  in a within-subject  
82 design of i.p. radiotracer administration. Finally, experiment 4 compared  $K_i^{mod}$  values obtained by the two  
83 routes of administration in a mouse model of hyperdopaminergia induced by sub-chronic ketamine  
84 administration. Our results show that i.p. administration of [<sup>18</sup>F]-FDOPA leads to good brain uptake of the  
85 radiotracer, moderate test-retest validity, and measurement of dopamine synthesis capacity comparable to  
86 the i.v. administration route. Intraperitoneal administration of [<sup>18</sup>F]-FDOPA thus enables longitudinal studies,  
87 refined methods to support more humane animal research, and has translational value in aiding  
88 development of novel therapies to treat dopamine dysfunction.

89

90 **Methods:**

91 **Subjects**

92 Male wildtype C57BL/6J mice, aged 6-7 weeks old upon arrival, were obtained from Charles River (Kent, UK)  
93 and housed in groups of up to 4 under a 12:12 hour light dark cycle with food and water provided *ad libitum*.  
94 Animals were habituated for a minimum of 1 week, before being used in procedures at a minimum age of 8  
95 weeks; the overall weight range of animals used in this study was 19-34 g (26.0±2.6 g) and animals were  
96 randomly assigned to different experiments and treatment groups. All animal experimental procedures were  
97 performed in accordance with the UK Animals (Scientific Procedures) Act 1986 and EU directive 2010/63/EU,  
98 and protocols were also approved by Invicro and Imperial College Animal Welfare and Ethical Review Body.

99

100 **Experimental Design**

101 Experiment 1 compared [<sup>18</sup>F]-FDOPA uptake kinetics between i.v. (N=12) and i.p. (N=13) routes of  
102 administration of the radiotracer. Experiments were performed in naïve mice weighing 19-34 g (25.9±3.3 g).  
103 Following a bolus injection of 1-19 MBq (8.4±5.6 MBq; 0.040±0.010 GBq/μmol), PET acquisition was carried  
104 out for 120 minutes. All mice subjected to an [<sup>18</sup>F]-FDOPA scan with i.p. injection of the radiotracer were  
105 allowed to recover at the end of the scan, monitored for 2 days to ensure their welfare and, following an  
106 interval of at least 2 days, were reused for subsequent longitudinal scanning in experiment 2 (N=7) or  
107 experiment 3 (N=6).

108 Experiment 2 compared  $Ki^{Mod}$  following i.p. or i.v. [<sup>18</sup>F]-FDOPA injection using a within-subject design.  
109 Following an interval of at least 12 days, a subset (N=7) of the animals recovered from the i.p. injected group  
110 in experiment 1 were subjected to a second [<sup>18</sup>F]-FDOPA scan using i.v. administration of the radiotracer.  
111 Animals used for this comparison weighed 25-34g (29.0±2.7 g). Following a bolus injection of 2-13 MBq  
112 (7.3±3.5 MBq; 0.039±0.0084 GBq/μmol), PET acquisition was carried out for 120 minutes.

113 Experiment 3 evaluated the test-retest estimation of  $Ki^{Mod}$  in a within-subject design of i.p. radiotracer  
114 administration. Following an interval of 2 days, a subset (N=6) of mice recovered from the i.p. injected group  
115 in experiment 1 were subjected to a second [<sup>18</sup>F]-FDOPA scan using i.p. administration of the radiotracer.  
116 Mice used in this comparison weighed 22-25 g (23.7±1.1 g). Following a bolus injection of 5-25 MBq (14.9±5.5  
117 MBq; 0.048±0.0058 GBq/μmol), PET acquisition was carried out for 120 minutes.

118 Experiment 4 compared  $Ki^{Mod}$  values obtained by the two routes of administration in a mouse model of  
119 hyperdopaminergia induced by sub-chronic ketamine administration as described previously [24]. In brief,  
120 mice received a daily i.p. injection for 5 consecutive days of 30 mg/kg ketamine (Sigma-Aldrich, K2753)  
121 dissolved in saline (KET, N=24) or were left untreated (Ctrl, N=23). Following an interval of 2 days after the  
122 last ketamine injection, animals were subjected to a single [<sup>18</sup>F]-FDOPA scan using either i.v. or i.p.  
123 administration of the radiotracer. Animals in this study weighed 21-32 g (25.9±2.0 g). Following a bolus  
124 injection of 2-23 MBq (9.0±4.8 MBq; 0.043±0.012 GBq/μmol), PET acquisition was carried out for 120 minutes  
125 (i.v.) or 140 minutes (i.p.).

126

127 **PET Acquisition**

128 [<sup>18</sup>F]-FDOPA was synthesised as described previously in the supplementary material published by Jauhar et  
129 al, 2017 [3]. One hour prior to administration of [<sup>18</sup>F]-FDOPA, mice were anaesthetised with isoflurane to  
130 undergo cannulation, and were maintained under isoflurane anaesthesia at 1-2% in 1L/min oxygen for the

131 duration of the study, with respiration rate and body temperature being monitored continuously throughout  
132 (BioVet, m2m Imaging Corp, OH, USA). To allow radiotracer delivery, either the external jugular vein was  
133 cannulated 45 minutes prior to scanning, or an intraperitoneal cannula was inserted 30 minutes before the  
134 scan. In order to prevent peripheral metabolism of the [<sup>18</sup>F]-FDOPA, inhibitors of catechol-O-methyl-  
135 transferase (COMT) and aromatic amino acid decarboxylase (AADC), Entacapone (40 mg/kg; Sigma-Aldrich,  
136 SML0654) and Benserazide hydrochloride (10 mg/kg; Sigma-Aldrich, B7283) were given intraperitoneally,  
137 respectively, at 45 minutes and 30 minutes prior to administration of [<sup>18</sup>F]-FDOPA [22-24]. To ensure optimal  
138 absorption of these inhibitors and the radiotracer, and to avoid competition with uptake of other neutral  
139 amino acids in diet across the blood-brain barrier (BBB) [24, 26], animals were food-deprived for 45 minutes  
140 before being anaesthetised. After administration of the inhibitors, mice underwent a 10 min CT scan in an  
141 Inveon PET/CT scanner (Siemens, Surrey, UK) to allow for attenuation correction of the PET signal. A dynamic  
142 PET scan was started concomitantly with bolus injection of [<sup>18</sup>F]-FDOPA and data was collected for up to 140  
143 minutes.

144

### 145 **PET Image Processing**

146 Following PET acquisition, data were histogrammed into 43 frames (10 x 3 s, 6 x 5 s, 8 x 30 s, 5 x 60 s, 6 x 300  
147 s, 8 x 600 s) for PET scans lasting 120 minutes. In the case of scans acquired for 140 minutes (Experiment 4,  
148 i.p. injected group), two additional frames of 600s were included. Data were reconstructed using filtered  
149 back projection with CT attenuation correction, adjusting for random noise, scatter, and radiotracer decay.  
150 Image processing was carried out using the Inveon Research Workspace (Siemens, USA), where the CT image  
151 was co-registered to the reconstructed PET image and checked for alignment. For each subject, the  
152 percentage-injected dose was normalised for body weight and injected activity to provide standardised  
153 uptake values (SUV). Regions of interest (ROI) with predefined shape and size were drawn manually on  
154 summation radioactivity images around the left and right striata (square; 0.07 cm<sup>3</sup> each) and the cerebellum  
155 (rectangular; 0.1 cm<sup>3</sup>) to extract time-activity curves (TACs) guided by CT and mouse brain anatomy [27].

156

### 157 **Extended Patlak Analysis**

158 Kinetic analyses were performed using an in-house pipeline in MATLAB version R2020a (MathWorks, MA,  
159 USA). Extended Patlak graphical analysis was used to determine the rate constant  $K_i^{Mod}$  (min<sup>-1</sup>), which  
160 provides an estimate for the rate of [<sup>18</sup>F]-FDOPA striatal uptake and its subsequent conversion into [<sup>18</sup>F]-  
161 fluoro-dopamine ([<sup>18</sup>F]-dopamine, or [<sup>18</sup>F]-FDA).  $K_i^{Mod}$  is a modified version of the influx rate constant  $K_i^{Cer}$   
162 (min<sup>-1</sup>), and takes into account an estimation of  $k_{loss}$  (min<sup>-1</sup>), the rate at which signal is removed from the  
163 system due to metabolism of [<sup>18</sup>F]-FDA, as described previously [22, 28-31]. In brief, peripherally  
164 administered [<sup>18</sup>F]-FDOPA is transported across the BBB to be taken up into striatal-projecting dopamine  
165 neurons, and is converted by AADC into [<sup>18</sup>F]-FDA, which then becomes irreversibly trapped in brain tissue  
166 [30, 32]. The rate at which [<sup>18</sup>F]-FDOPA is taken up and converted into [<sup>18</sup>F]-FDA is used as an index of  
167 presynaptic dopamine synthesis capacity. This rate constant is referred to as  $K_i^{Cer}$  when the cerebellum is  
168 used as a reference region in place of an arterial input function. The ratio between irreversibly trapped  
169 radiotracer measured in the striatum *versus* free radiotracer in the reference cerebellum region takes on a  
170 linear relationship when plotted against the ratio of running time integral of cerebellum SUV and cerebellar  
171 SUV, a function referred to as stretch time. The slope of this linear plot as derived by graphical Patlak analysis  
172 [33] corresponds to the influx rate constant  $K_i^{Cer}$ . In humans, [<sup>18</sup>F]-FDA trapping is considered irreversible for  
173 up to two hours after [<sup>18</sup>F]-FDOPA administration [32]. Rodents have a much faster metabolic rate and [<sup>18</sup>F]-

174 FDA is lost through metabolism during typical scan durations [21, 22], resulting in a deviation from the linear  
175 relationship between striatal uptake and stretch time. This can be corrected for using an extended Patlak  
176 analysis, which provides a modified influx rate constant,  $K_i^{mod}$ , that estimates the metabolism of [ $^{18}\text{F}$ ]-FDA as  
177 rate of loss,  $k_{loss}$ , and adjusts for it to restore the linear relationship [24, 29, 30].

178

### 179 **Optimal Window for Determining $K_i^{Mod}$ and $k_{loss}$ Parameters**

180 Accurate estimation of the  $K_i^{Mod}$  parameter requires the acquisition of sufficient temporal data so as to  
181 capture the reversible nature of the kinetics present in the system. Subsequently,  $k_{loss}$  is determined as the  
182 deviation from the linear regression over time. This makes estimation of these two parameters sensitive to  
183 the time range chosen to carry out the analysis. To establish the optimal window for determining  $K_i^{Mod}$  and  
184  $k_{loss}$  parameters, individual TAC data, acquired following i.p. radiotracer administration in experiment 1  
185 (N=13, acquired up to 120 minutes) and experiment 4 (naïve group only, N=12, acquired up to 140 minutes)  
186 was processed through the extended Patlak analysis using varying start ( $T^*$ ) and end times ( $T^{end}$ ). For each  
187 parameter, the standard deviation (S.D.) for  $K_i^{Mod}$  and  $k_{loss}$ , and the coefficient of variation (%CV) were  
188 calculated at the different time points to identify the analysis window that produced the least within-group  
189 variability. Using these measures, the optimal time range for analysis of  $K_i^{Mod}$  and  $k_{loss}$  following i.v.  
190 administration was previously determined to be 15-120 minutes [23]; in the current study the effect of  
191 altering time windows on both parameters was tested for i.p. administration.

192

### 193 **Statistical analysis**

194 Statistical tests were carried out using GraphPad Prism v9 (GraphPad Software, La Jolla, California, USA).  
195 Average numerical values in the text are expressed as mean  $\pm$  S.D.; in graphs, data are shown as mean  $\pm$  S.D..  
196 Data were tested for statistical outliers using ROUT test, Q=0.5%, and tested for normal distribution using  
197 the Kolmogorov-Smirnov test to decide on the use of parametric (t-test) or nonparametric tests; no statistical  
198 outliers were identified, and all data showed a normal distribution. Slopes of SUVR curves were compared  
199 using simple linear regression analysis. Statistical tests used are specified in the text and figure legends.

200

201 **Results**

202

203 **Experiment 1: [<sup>18</sup>F]-FDOPA striatal uptake in the mouse brain is similar following either i.p. or i.v.**  
204 **radiotracer injection**

205 **Comparison of radiotracer uptake**

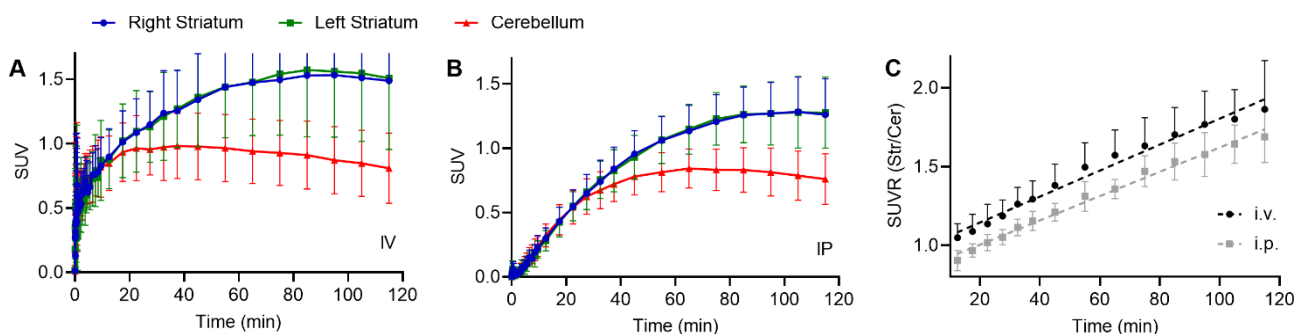
206 The weight of animals scanned did not significantly differ between groups (i.p., 26.8±3.6 g; i.v., 24.7±2.4 g;  
207 p=0.12, t=1.62, unpaired two-tailed t-test). However, the dose injected in the i.v. group was lower than in  
208 the i.p. group due to the more restrictive injectable volume using i.v. administration (i.p., 0.45±0.23 MBq/g;  
209 i.v., 0.17±0.10 MBq/g; p=0.0018, t=3.574, unpaired two-tailed t-test).

210 The TACs revealed different dynamics of uptake of the [<sup>18</sup>F]-FDOPA radiotracer depending on the injection  
211 method (Fig.1A-B). Neither method showed a difference in standard uptake value (SUV) of the radiotracer  
212 between the left and right striatum (Str) (i.v.: p=0.54, t=0.62; i.p.: p=0.72, t=0.36; paired two-tailed t-test).  
213 The time to reach the highest level of radiotracer trapping in the striatum (SUV<sub>PEAK</sub>) was slightly delayed  
214 following i.p. injection (Fig.1B) as compared to i.v. injection (Fig.1A), but this did not reach statistical  
215 significance (i.v.: 88.8 ± 11.7 min; i.p.: 95.4 ± 14.6 min; p=0.084, t=1.77, unpaired two-tailed t-test). Peak  
216 striatal SUV levels were reduced following i.p. injection as compared to i.v. injection (SUV<sub>PEAK, IV</sub>, 1.59 ± 0.49;  
217 SUV<sub>PEAK, IP</sub>, 1.32 ± 0.26; p=0.017, t=2.47, unpaired two-tailed t-test).

218 In the cerebellum (Cer), where binding of the radiotracer is assumed to be non-specific and the kinetics are  
219 highly reversible, washout started at an earlier time point after radiotracer delivery as compared to the  
220 striatum: for both methods, the cerebellar SUV<sub>PEAK</sub> was reached significantly earlier than the striatal SUV<sub>PEAK</sub>  
221 (i.v.<sub>Cer</sub>, 36.2 ± 9.9 min, i.v.<sub>Str</sub>, 88.8 ± 11.7 min, p<0.001, t=13.3; i.p.<sub>Cer</sub>, 75.8 ± 17.1 min, i.p.<sub>Str</sub>, 95.4 ± 14.6 min,  
222 p<0.001, t=3.75; unpaired two-tailed t-tests). Furthermore, cerebellar SUV<sub>PEAK</sub> was reached significantly later  
223 following i.p. administration as compared to i.v. administration (i.v.<sub>Cer</sub>, 36.2 ± 9.9 min, i.p.<sub>Cer</sub>, 75.8 ± 17.1 min,  
224 p<0.001, t=7.00, unpaired two-tailed t-test). Peak activity levels were significantly lower in the cerebellum  
225 than in the striatum for both methods (i.v.: SUV<sub>PEAK, Cer</sub>, 1.01 ± 0.25, SUV<sub>PEAK, Str</sub>, 1.59 ± 0.49, p<0.001, t=3.82;  
226 i.p.: SUV<sub>PEAK, Cer</sub>, 0.87 ± 0.18, SUV<sub>PEAK, Str</sub>, 1.32 ± 0.26, p<0.001, t=5.63; unpaired two-tailed t-tests). There was  
227 no significant difference in cerebellar SUV<sub>PEAK</sub> values between the two methods (p=0.12, t=1.64, unpaired  
228 two-tailed t-test).

229 The ratio between striatal and cerebellar SUV (SUV<sub>R</sub>) over time is shown for both methods in Fig.1C. Despite  
230 reduced overall SUV<sub>R</sub> values following i.p. administration, there was no significant difference in slope of the  
231 linear fit to the SUV<sub>R</sub> (calculated for 10-120 minutes) between the two methods (i.v., slope 0.0082 ± 0.00038,  
232 R<sup>2</sup>=0.74; i.p., slope 0.0077 ± 0.00021, R<sup>2</sup>=0.88; p=0.21, F=1.58).

233 All mice subjected to an [<sup>18</sup>F]-FDOPA scan with i.p. injection of the radiotracer (N=13) made an unremarkable  
234 recovery, enabling their re-use for longitudinal studies.



235



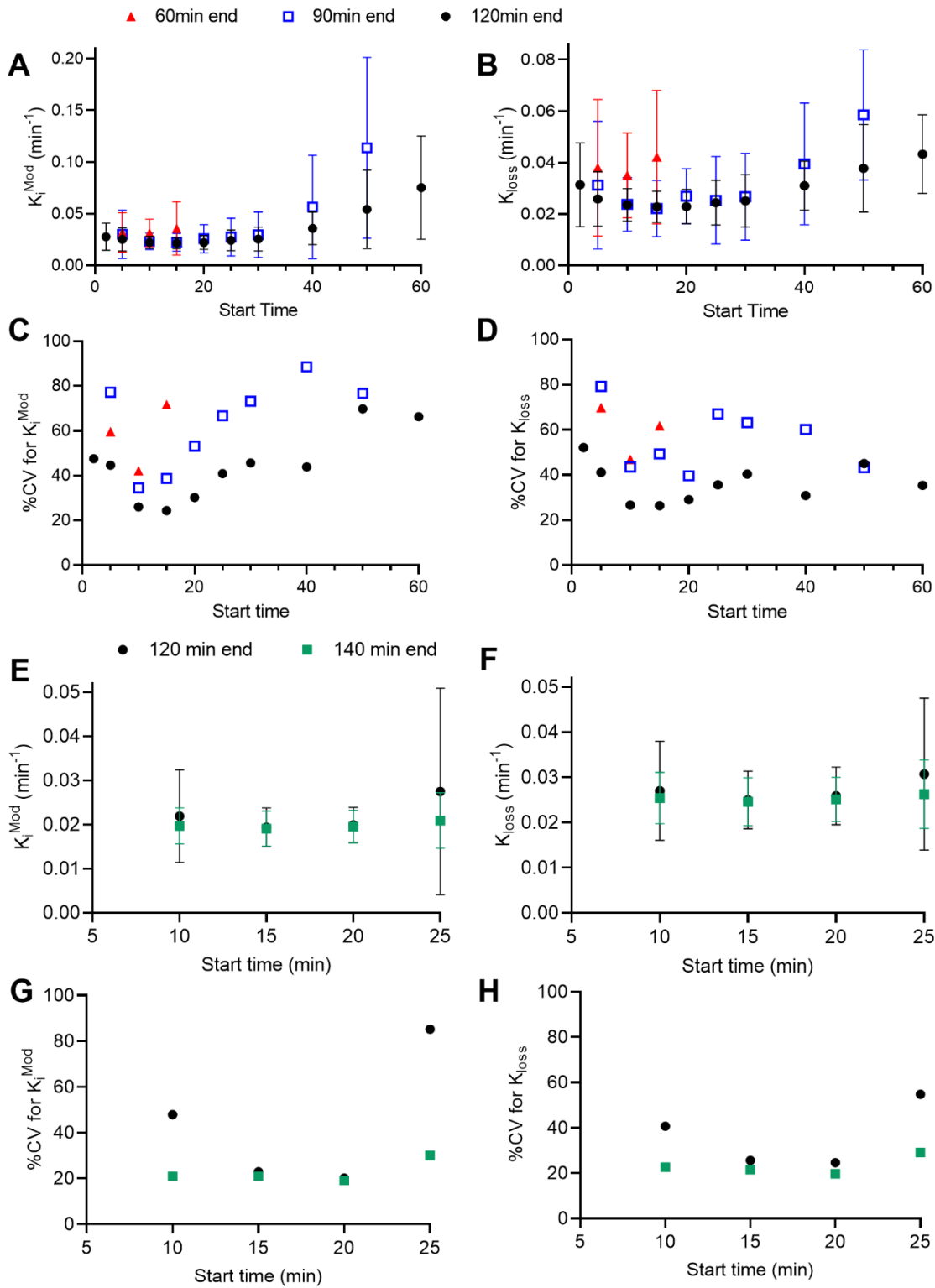
236 **Figure 1: Time-activity curves and SUVR showing the effect of the radiotracer injection method on [<sup>18</sup>F]-**  
237 **FDOPA uptake and loss over time. A,B.** TAC showing SUV of [<sup>18</sup>F]-FDOPA activity over time within the right  
238 striatum (blue circles), left striatum (green squares) and cerebellum (red triangles) following intravenous (A,  
239 i.v., N=12) or intraperitoneal (B, i.p., N=13) administration. Values are mean  $\pm$  S.D.. C. SUVR Ratio (SUVR)  
240 between striatum (Str) and cerebellum (Cer) over time following i.v. or i.p. injection. Dashed lines show the  
241 best-fit linear regression. Values are mean  $\pm$  S.D..

242

#### 243 The effect of analysis window on $K_i^{Mod}$ and $k_{loss}$ Parameters

244 Variation of  $T^*$  and  $T^{end}$  in the Patlak analysis of i.p. administered [<sup>18</sup>F]-FDOPA TACs showed that both the  
245 modified influx rate constant  $K_i^{Mod}$ , and the loss rate constant  $k_{loss}$ , as well as the variability within each group,  
246 were altered in response to changes in the analysis window (Fig.2A-B).  $K_i^{Mod}$  and  $k_{loss}$  could not be determined  
247 for analysis window lengths of 30 minutes or less, as in those cases the estimation of  $k_{loss}$  would be based on  
248 4 or less points to identify the linear range of the Patlak plot. The percentage coefficient of variation (%CV)  
249 for both the  $K_i^{Mod}$  and  $k_{loss}$  parameters decreased with increasing  $T^{end}$ , with the least intra-group variability  
250 seen with an analysis window of 15-120 minutes ( $T^*$  and  $T^{end}$ , respectively) (%CV  $K_i^{Mod}$ , 24.4%; %CV  $k_{loss}$ ,  
251 26.4%; Fig.2C-D). Consistently, at this time window, the S.D. for both  $K_i^{Mod}$  and  $k_{loss}$  is lowest (Fig.2A-B),  
252 suggesting the greatest degree of consistency across samples. This is identical to the analysis window  
253 optimised for i.v. administration of [<sup>18</sup>F]-FDOPA in previous work [23].

254 Due to the slower uptake kinetics following i.p. radiotracer administration, resulting in a shorter time window  
255 available for the estimation of  $k_{loss}$ , we verified in a separate dataset (N=12 naïve animals) whether extending  
256 the scan time, and therefore the analysis window used for the estimation of  $K_i^{Mod}$  and  $k_{loss}$  by extended Patlak  
257 analysis, to 140 minutes could further reduce within-group variability of  $K_i^{Mod}$  and  $k_{loss}$ . Assessment of a  
258 limited set of  $T^*$  values showed that at a  $T^{end}$  of 140 minutes, within-group variability and %CV are less  
259 sensitive to variation in  $T^*$  than when using a  $T^{end}$  of 120 minutes, and an analysis window of 20-140 minutes  
260 yielded slightly reduced variability compared to 15-120 minutes (%CV  $K_i^{Mod}$ , 19.1%; %CV  $k_{loss}$ , 19.7%; Fig.2E-  
261 H). Therefore, the analysis window of 20-140 minutes was chosen for analysis of scan data acquired up to  
262 140 minutes following i.p. administration of [<sup>18</sup>F]-FDOPA, whereas an analysis window of 15-120 minutes was  
263 selected as most optimal for datasets acquired up to 120 minutes.



264

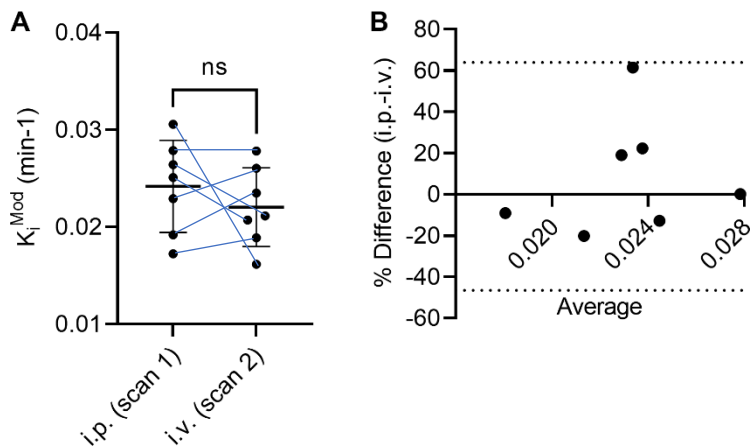
265 **Figure 2: Effect of varying  $T^*$  and  $T^{end}$  on  $K_i^{Mod}$  and  $k_{loss}$  values and inter-sample variability following i.p.**  
 266 **radiotracer administration. A,B.** Values calculated from TACs following i.p. radiotracer administration (N=13)  
 267 by extended Patlak analysis for  $K_i^{Mod}$  (A) and  $k_{loss}$  (B) with variable  $T^*$  (x-axis) and  $T^{end}$  (60 min: red triangles;  
 268 90 min: blue open squares; 120 min: black circles). Values are mean  $\pm$  S.D.. C,D. %CV for  $K_i^{Mod}$  (C) and  $k_{loss}$  (D)  
 269 with variable  $T^*$  and  $T^{end}$ . E-H. As A-D, but showing the effect of varying  $T^*$  (x-axis) on  $K_i^{Mod}$  (E) and  $k_{loss}$  (F)  
 270 outcome values and S.D. as well as %CV for  $K_i^{Mod}$  (G) and  $k_{loss}$  (H) using a  $T^{end}$  of 120 min (black circles) or 140  
 271 min (green squares).

272

273 **Experiment 2: Within-subject comparison shows no effect of radiotracer administration route on  $K_i^{Mod}$**   
274 **value.**

275 Mice underwent two scanning sessions, the first scan following i.p. administration of [ $^{18}$ F]-FDOPA, and the  
276 second scan following i.v. administration of the radiotracer, with an interval of at least 12 days between  
277 scans. Animals did not significantly differ in weight in consecutive scans (i.p., first scan, 29.1 $\pm$ 3.6 g; i.v., second  
278 scan, 28.8 $\pm$ 1.8 g;  $p=0.84$ ,  $t=0.22$ , paired two-tailed t-test) or in injected dose (i.p., first scan, 0.28 $\pm$ 0.14 MBq/g;  
279 i.v., second scan, 0.23 $\pm$ 0.10 MBq/g;  $p=0.48$ ,  $t=0.75$ , paired two-tailed t-test).

280 There was no significant difference between mean  $K_i^{Mod}$  derived from either method (Fig.3A; i.p.,  
281 0.024 $\pm$ 0.0047 min $^{-1}$ ; i.v., 0.022 $\pm$ 0.0041 min $^{-1}$ ;  $p=0.42$ ,  $t=0.87$ , two-tailed paired t-test) and the coefficient of  
282 variation was comparable (i.p., 19.6%; i.v., 18.4%). Likewise, there was no difference in  $k_{loss}$  derived from  
283 either method (i.p., 0.024 $\pm$ 0.0056 min $^{-1}$ ; i.v., 0.023 $\pm$ 0.0040 min $^{-1}$ ;  $p=0.69$ ,  $t=0.42$ , paired two-tailed t-test;  
284 %CV i.p., 23.1%; %CV i.v., 17.0%; data not shown). Comparison of the methods by a Bland-Altman plot (Fig.3B)  
285 showed a bias of 8.7 $\pm$ 28.2% towards i.p. administration, however this finding did not indicate a consistent  
286 bias. However the order of scans was not counterbalanced and that is a limitation of this experiment.



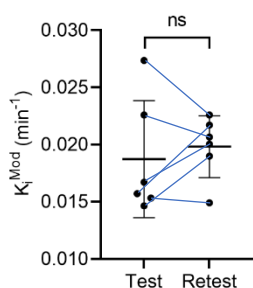
287  
288 **Figure 3: Within-animal comparison of  $K_i^{Mod}$  outcome values. A.**  $K_i^{Mod}$  calculated using 15-120 min of the TAC  
289 and extended Patlak analysis. Values are mean  $\pm$  S.D.;  $N=7$ ; ns, not significant, paired two-tailed t-test. **B.**  
290 Comparison of  $K_i^{Mod}$  outcome values using a Bland-Altman plot to estimate bias. Dotted lines indicate the 95%  
291 limits of agreement.

292  
293 **Experiment 3: Test-retest reliability of striatal dopamine synthesis capacity to validate the use of i.p.**  
294 **administration of [ $^{18}$ F]-FDOPA for longitudinal studies**

295 Mice underwent two scanning sessions following i.p. administration of [ $^{18}$ F]-FDOPA, with an interval of 2 days  
296 between scans. Between consecutive scans, animals did not significantly differ in weight (first scan, 24.2 $\pm$ 0.7  
297 g; second scan, 23.3 $\pm$ 1.2 g;  $p=0.0644$ ,  $t=2.37$ , paired two-tailed t-test) or in injected dose (first scan, 0.64 $\pm$ 0.12  
298 MBq/g; second scan, 0.61 $\pm$ 0.31 MBq/g;  $p=0.77$ ,  $t=0.31$ , paired two-tailed t-test).

299 There was no significant difference between mean  $K_i^{Mod}$  for subsequent scans (Fig.4A; test, 0.0187 $\pm$ 0.0051  
300 min $^{-1}$ , retest, 0.0198 $\pm$ 0.0027 min $^{-1}$ ;  $p=0.54$ ,  $t=0.65$ , paired two-tailed t-test), although the coefficient of  
301 variation was reduced in the retest scans (test, 27.3%; retest, 13.7%). Likewise, there was no difference in  
302  $k_{loss}$  derived from either method (test, 0.021 $\pm$ 0.0070 min $^{-1}$ ; retest, 0.016 $\pm$ 0.0030 min $^{-1}$ ;  $p=0.13$ ,  $t=1.83$ , paired  
303 two-tailed t-test; %CV test, 33.3%; %CV retest, 18.3%; data not shown). Using the two-way mixed model with  
304 absolute agreement, the intraclass correlation coefficient (ICC) for  $K_i^{Mod}$  was 0.515, which indicated a

305 moderate correlation between the two datasets [34]. Likewise, the percentage absolute variability (%VAR)  
 306 indicated moderate reliability (%VAR=17.8 ± 10.7%).



307

308 **Figure 4: Test-retest reliability of  $K_i^{Mod}$  outcome values.**  $K_i^{Mod}$  calculated using 15-120 minutes of the TAC and  
 309 extended Patlak analysis. Values are mean ± S.D.; N=6; ns, not significant, paired two-tailed t-test.

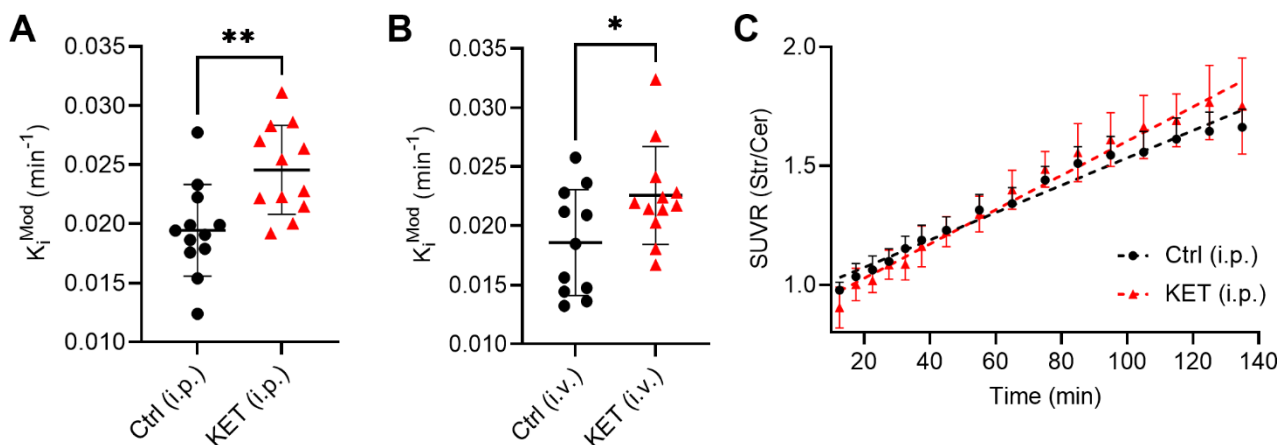
310

311 **Experiment 4: Elevated dopamine synthesis capacity following sub-chronic ketamine can be reproduced**  
 312 **using either i.p. or i.v. [ $^{18}$ F]-FDOPA administration**

313  $K_i^{Mod}$  values in naïve animals (Ctrl) versus animals that received sub-chronic ketamine administration (KET)  
 314 were compared following a single scan using either i.p. or i.v. [ $^{18}$ F]-FDOPA administration. There was no  
 315 significant difference between treatment groups in animal weight (naïve, 26.3±2.3 g; KET, 25.5±1.8 g; p=0.18,  
 316 t=1.38, unpaired two-tailed t-test) or injected dose (naïve, 0.30±0.15 MBq/g; KET, 0.39±0.20 MBq/g; p=0.064,  
 317 t=1.90, unpaired two-tailed t-test).

318 A significant increase in  $K_i^{Mod}$  was observed following sub-chronic ketamine administration as compared to  
 319 naïve animals, using either i.p. administration (Fig.5A, Ctrl, 0.019±0.0039 min<sup>-1</sup>, KET, 0.025±0.0038 min<sup>-1</sup>;  
 320 p=0.0035, t=3.28, unpaired two-tailed t-test) or i.v. administration (Fig.5B, Ctrl, 0.019±0.0045 min<sup>-1</sup>, KET,  
 321 0.023±0.0041 min<sup>-1</sup>, p=0.037, t=2.22). For both methods, the difference was observed with large effect size  
 322 (i.p.: Cohen's d=1.34; i.v., Cohen's d=0.93). The slope of the striatal/cerebellar SUVR following i.p.  
 323 administration of the radiotracer was significantly increased in ketamine-treated animals as compared to  
 324 naïve animals (Fig.5C) (naïve, slope 0.0057 ± 0.00014, R<sup>2</sup>=0.90; KET, slope 0.0072 ± 0.00020, R<sup>2</sup>=0.87; p<0.001,  
 325 F=35.74). A significant increase in  $k_{loss}$  was observed following sub-chronic ketamine administration as  
 326 compared to naïve animals, using i.v. administration (Ctrl, 0.01696±0.0062 min<sup>-1</sup>, KET, 0.022±0.0039 min<sup>-1</sup>;  
 327 p=0.0285, t=2.35, unpaired two-tailed t-test). However no significant increase in  $k_{loss}$  was observed using i.p.  
 328 administration (Ctrl, 0.02515±0.0052 min<sup>-1</sup>, KET, 0.0269±0.0059 min<sup>-1</sup>; p=0.4491, t=0.77, unpaired two-tailed  
 329 t-test) driven by the control group's relatively higher  $k_{loss}$  value.

330



331 **Figure 5. The effect of sub-chronic ketamine administration on dopamine synthesis capacity measured by**  
332 **two different routes of [<sup>18</sup>F]-FDOPA administration. A,B**  $K_i^{Mod}$  calculated using 20-140 minutes of the TAC  
333 and extended Patlak analysis following i.p. administration **(A)** or 15-120 minutes of the TAC following i.v.  
334 administration **(B)** of [<sup>18</sup>F]-FDOPA in naïve (Ctrl) or ketamine-treated (KET) animals. Values are mean  $\pm$  S.D.;  
335 N=12 (Ctrl, i.p.; KET, i.p.; KET, i.v.) or N=11 (Ctrl, i.v.); \*p<0.05, \*\*p<0.01, unpaired two-tailed t-tests. **C.** SUVR  
336 over time in Ctrl or KET animals and following i.p. administration of [<sup>18</sup>F]-FDOPA. Dashed lines show the best-  
337 fit linear regression. Values are mean  $\pm$  S.D..

338

339 **Discussion:**

340 In the current study, we evaluated the use of i.p. administration of [<sup>18</sup>F]-FDOPA in comparison to i.v.  
341 administration in mice for the assessment of dopamine synthesis capacity in the striatum. Our data show  
342 that i.p. administration is a method that allows excellent striatal radiotracer uptake, with moderate test-  
343 retest reliability [34], a similar range of outcome values as compared to i.v. administration, and fast and  
344 unremarkable recovery of the animals following imaging, enabling longitudinal studies and within-animal  
345 comparison. Importantly, using i.p. [<sup>18</sup>F]-FDOPA administration, we were able to reproduce previously  
346 measured enhanced dopamine synthesis in a mouse model of hyperdopaminergia [24]. Our results are in  
347 agreement with previous studies in rodents where <sup>18</sup>F-sodium fluoride (<sup>18</sup>F-NaF) and <sup>18</sup>F-fludeoxyglucose (<sup>18</sup>F-  
348 FDG) radiotracers showed comparable results between i.v. and i.p. administration routes [35, 36].

349 We applied an extended Patlak analysis for the determination of dopamine synthesis capacity following i.p.  
350 [<sup>18</sup>F]-FDOPA administration in mice, showing that both  $k_{loss}$  and the modified influx rate constant  $K_i^{Mod}$  are  
351 sensitive to the start and end times of the analysis window. The derivation of  $K_i^{Mod}$  is dependent on the  
352 estimation of  $k_{loss}$  and so using the analysis range that provided the most consistent estimate for  $k_{loss}$  also  
353 yielded the least variable estimates of  $K_i^{Mod}$ . Previously, Holden et al. (1997) demonstrated in non-human  
354 primates that with a longer scan duration (end time of 240 minutes) the  $k_{loss}$  parameter is insensitive to the  
355 start time [29]. With longer scan duration there are more data available with which to derive an accurate  
356 measure of  $k_{loss}$ . Likewise, we found that extending the scan time from 120 to 140 minutes reduced sensitivity  
357 of  $K_i^{Mod}$  and  $k_{loss}$  for variation in T\* (Fig.2). Due to the complexity of maintaining mice under anaesthesia for  
358 an extended period, further lengthening of scan time is not desirable, particularly when recovering the animal  
359 after imaging. In the present study we found that the 20-140 minute analysis window provided the lowest  
360 within-group variability over the time range tested (%CV  $K_i^{Mod}$ = 19%, %CV  $k_{loss}$ = 20%, Fig.2G-H). This is a slight  
361 increase as compared to 11% in rats at 180 minutes scan duration, where the radiotracer was injected i.v. in  
362 the tail [22]. As expected, with shorter scan lengths (up to 120 minutes), within-group variability in our study  
363 increased to over 40% (Fig.2C-D); such high variability would potentially restrict the use of this method to  
364 studies with only very large expected between-group effect sizes.

365 With similar inter-group variability as reported here, future mouse studies using the extended Patlak analysis  
366 would require group sizes of at least 10 to detect effect sizes of the same magnitude as the effect we found  
367 for ketamine (d=1.4) with >90% power. This can be reduced to N=7 for studies where two within-subject  
368 measurements are possible, thus i.p. administration of [<sup>18</sup>F]-FDOPA could support the reduction of subject  
369 numbers in rodent PET imaging studies.

370 In the present study we have used a group-housed inbred strain of mouse to reduce within-group individual  
371 variability and provide greater resolution of the impact of different analysis start and end times, as well as  
372 support reproducibility in the test-retest reliability study and the within-subject comparison of i.p. and i.v.  
373 administration of [<sup>18</sup>F]-FDOPA. The within-group variability obtained in our study (19%) is somewhat higher  
374 than that seen in human [<sup>18</sup>F]-FDOPA PET imaging studies, where variability in  $K_i^{Cer}$  was 10% in the whole  
375 striatum, with a range of 6-12% in striatal sub-regions [37]. Likewise, the test-retest reliability (ICC=0.52 and  
376 %VAR=18%) in our study is somewhat lower than that reported in humans (ICC=0.84 and %VAR=4.5% in  
377 human striatum) [37]. These differences probably reflect the far larger size of the striatum in humans, which  
378 results in higher resolution images and makes correct placement of the ROI more reliable and reproducible  
379 than in mice. Nevertheless, the ICC value in mice indicates moderate reliability [34], supporting the use of  
380 this approach.

381 To our knowledge, we are the first group to apply extended Patlak analysis to mice scanned with [<sup>18</sup>F]-FDOPA,  
382 although others have used the radiotracer in mice to measure overall radiotracer binding at a predefined

383 timepoint after radiotracer injection [38-40]. Although these studies revealed increased radiotracer binding  
384 in the striatum as compared to other brain regions, reliability of this parameter has not been assessed in  
385 those studies. A major advantage of kinetic modelling using Patlak analysis is that outcome values correspond  
386 directly to those used in human [<sup>18</sup>F]-FDOPA PET imaging [10, 41]. SUVR is an alternative proxy measure that  
387 has been used to measure dopamine synthesis capacity in humans [42]. Our data provide a preliminary  
388 indication that this output value may also be used as an alternative to  $K_i^{Mod}$  in assessment of dopamine  
389 function using [<sup>18</sup>F]-FDOPA PET imaging and i.p. radiotracer administration in mice (Fig. 5C).

390 The  $k_{loss}$  values determined by our approach, both the i.v. and i.p. method is similar to comparable  
391 parameters determined in rats [43] and humans [44] in previous studies but it has been determined to be an  
392 order lower in non-human primates [30, 31, 45]. There are no comparator studies in mice with the exception  
393 of an earlier publication from our group and are most likely related to the species in which they are measured  
394 [23]. A methodological consideration for [<sup>18</sup>F]-FDOPA PET scanning in rodents is that administration of COMT  
395 and AADC inhibitors is required to prevent peripheral metabolism of the radiotracer, and that between-  
396 subject variability in the uptake of these inhibitors underlie variability in the data. The intraperitoneal  
397 injection of these inhibitors just prior to intraperitoneal radiotracer injection may introduce additional  
398 variability in radiotracer uptake as compared to intravenous injection. The large surface area of the  
399 peritoneal membrane aids rapid absorption, however, the radiotracer is predominantly expected to be  
400 transported to systemic circulation through the hepatic portal pathway [46]. Other drug-metabolising  
401 enzymes do not play a significant role in the breakdown of DOPA [47], and hence its brain kinetics suited our  
402 study. Peripheral inhibitors are also used in human [<sup>18</sup>F]-FDOPA imaging, supporting the translational value  
403 of this approach in mice [3, 6].

404 Importantly, using i.p. administration of [<sup>18</sup>F]-FDOPA, and in an independent cohort using i.v. administration,  
405 we were able to reproduce the previously observed increased dopamine synthesis rate in mice receiving sub-  
406 chronic administration of ketamine [24]. One potential limitation for the study on the effects of ketamine is  
407 that the control animals did not receive control injections, in contrast to the ketamine treated animals. Thus,  
408 the design cannot disambiguate whether it is the ketamine or injection that resulted in the group differences.  
409 However, the study by Kokkinou et al (2020) [24] used saline injections as the control condition, finding a  
410 significant difference with the ketamine group, indicating that the lack of control injections in our control  
411 group is unlikely to explain our finding. These results provide further evidence that ketamine has effects on  
412 the regulation of dopamine signalling. Furthermore, the high reproducibility of the effect supports the use of  
413 sub-chronic ketamine in mice to create a model of hyperdopaminergia as a proxy of the dopamine signalling  
414 abnormality associated with psychotic disorders [15]. Also the lower SUVR to cerebellum with i.p. than i.v.  
415 might mean that the i.p. approach is less sensitive to detect models of reduced dopamine synthesis capacity,  
416 although this effect may be offset by the lower variability with i.p. relative to i.v. Studies using models of  
417 reduced dopamine synthesis capacity are needed to evaluate this. It is also interesting to note that the mean  
418  $K_i$  values in experiment 2 are similar to those in ketamine exposed group in experiment 4. This may be an  
419 artefact of the smaller sample size in experiment 2, but could also reflect cohort differences, which highlights  
420 the value of longitudinal imaging.

421

422

## 423 **Conclusion**

424 In conclusion, we have demonstrated that intraperitoneal administration of [<sup>18</sup>F]-FDOPA provides a reliable  
425 measure of presynaptic dopamine synthesis capacity with similar values to those obtained with intravenous

426 injection. We also show that ketamine elevates dopamine synthesis capacity, extending previous findings to  
427 show this in an independent cohort of animals. Sub-chronic glutamate receptor antagonism using other  
428 pharmacological interventions has also shown to elevate dopamine synthesis capacity and elimination of  
429 [<sup>18</sup>F]-FDOPA in rodent and humans thus supporting our findings [44, 48]. Our i.p. administration model  
430 finding is consistent with elevated dopamine synthesis capacity while the high control group kloss in the i.p.  
431 model may have obscured differences in catabolism and so further studies are needed. However it must be  
432 mentioned that ketamine model mimics findings seen with the catabolism and elimination of [<sup>18</sup>F]-FDOPA  
433 in the brain of patients with schizophrenia [45]. Application of this method in mice will allow for longitudinal  
434 studies in mouse models that assess the effect genetic, pharmacological, and environmental changes on the  
435 dopamine system. The possibility of within-animal comparison allows for a reduction in animal numbers  
436 required, thereby supporting ethical standards in animal research to reduce usage of animals where possible.  
437 The method allows for translational measurement of presynaptic dopamine function, thereby providing an  
438 important tool in understanding the factors that may ultimately play a role in several neurological and  
439 psychiatric disorders as well as supporting the development of novel pharmacological treatments.

440



441 **Data availability**

442 The datasets generated and/or analysed in this study, as well as all code used in the present study, are  
443 available from the corresponding author upon reasonable request.

444

445 **Conflicts of interest**

446 The authors declare that there is no conflict of interest regarding the publication of this article.

447

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455

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459

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