

# Does nonlinear blood-brain barrier transport matter for (lower) morphine dosing strategies?

Gülave, B.; Budda, D.; Saleh, M.A.A.E.W.; Hasselt, J.G.C. van; Lange, E.C.M. de

### Citation

Gülave, B., Budda, D., Saleh, M. A. A. E. W., Hasselt, J. G. C. van, & Lange, E. C. M. de. (2023). Does nonlinear blood-brain barrier transport matter for (lower) morphine dosing strategies? *European Journal Of Pharmaceutical Sciences*, *187*. doi:10.1016/j.ejps.2023.106482

Version:Publisher's VersionLicense:Creative Commons CC BY 4.0 licenseDownloaded from:https://hdl.handle.net/1887/3638448

**Note:** To cite this publication please use the final published version (if applicable).

Contents lists available at ScienceDirect



## **European Journal of Pharmaceutical Sciences**

journal homepage: www.elsevier.com/locate/ejps

## Does nonlinear blood-brain barrier transport matter for (lower) morphine dosing strategies?

Berfin Gülave<sup>1</sup>, Divakar Budda<sup>1</sup>, Mohammed AA Saleh, JG Coen van Hasselt, Elizabeth CM de Lange<sup>\*</sup>

Division of Systems Pharmacology and Pharmacy, Leiden Academic Center for Drug Research, Leiden University, Leiden 2333 CC, the Netherlands

A R T I C L E I N F O	A B S T R A C T			
A R T I C L E I N F O Keywords: Morphine Blood-brain barrier Nonlinear LeiCNS-PK3.0	Morphine blood-brain barrier (BBB) transport is governed by passive diffusion, active efflux and saturable activ influx. This may result in nonlinear plasma concentration-dependent brain extracellular fluid (brain <sub>ECF</sub> ) pha macokinetics of morphine. In this study, we aim to evaluate the impact of nonlinear BBB transport on brain <sub>EC</sub> pharmacokinetics of morphine and its metabolites for different dosing strategies using a physiologically base pharmacokinetic simulation study. We extended the human physiologically based pharmacokinetic LeiCNS PK3.0, model with equations for nonlinear BBB transport of morphine. Simulations for brain <sub>ECF</sub> pharmacok netics were performed for various dosing strategies: intravenous (IV), oral immediate (IR) and extended releas (ER) with dose range of 0.25–150 mg and dosing frequencies of 1–6 times daily. The impact of nonlinear BB transport on morphine CNS pharmacokinetics was evaluated by quantifying (i) the relative brain <sub>ECF</sub> to plasm exposure (AUC <sub>u, brainECF</sub> /AUC <sub>u, plasma</sub> ) and (ii) the impact on the peak-to-trough ratio (PTR) of concentration-tim profiles in brain <sub>ECF</sub> and plasma. We found that the relative morphine exposure and PTRs are dose dependent for the evaluated dose range. The highest relative morphine exposure value of 1.4 was found for once daily 0.25 m ER and lowest of 0.1 for 6-daily 150 mg IV dosing. At lower doses the PTRs were smaller and increased wit increasing dose and stabilized at higher doses independent of dosing frequency. Relative peak concentrations of morphine in relation to its metabolites changed with increasing dose. We conclude that nonlinearity of morphin BBB transport affects the relative brain <sub>ECF</sub> exposure and the fluctuation of morphine and its metabolites mainly a lower dosing regimens.			

#### 1. Introduction

Morphine is an opioid with an important place for the treatment of acute and chronic pain. The main metabolites of morphine in humans are morphine-3-glucuronide (M3G) and morphine-6-glucuronide (M6G) (Christrup, 1997; De Gregori et al., 2012; Frölich et al., 2011). M3G displays a relatively low affinity for opioid receptors and has no analgesic activity. In fact, an opposite effect, hyperalgesia, has been reported (Frölich et al., 2011; Gabel et al., 2022). M6G, however, is capable of eliciting profound analgesic activity, and has even been propose to as the main drive of the analgesic effects of morphine treatment (Klimas and Mikus, 2014; Murthy et al., 2002).

Many pharmacological studies on morphine and its metabolites effect have been performed, but these studies have typically only considered its plasma pharmacokinetics and not the target site pharmacokinetics. However, morphine and its metabolites first need to cross the blood–brain barrier (BBB) to reach the brain extracellular fluid (brain<sub>ECF</sub>) where they can bind with opioid receptors in the brain. Thus, brain<sub>ECF</sub> concentrations, and not plasma concentrations, should therefore be considered the target site concentration driving the effect. The rate and extent of BBB transport of morphine, M3G, and M6G are different, as has been shown by microdialysis studies in rats. Beside passive transports, para- and transcellular, morphine, M3G and M6G are actively transported. For morphine, both the P-glycoprotein (P-gp) (Chaves et al., 2017; Letrent et al., 1999; Xie et al., 1999) and probenecid-sensitive transporters (Tunblad et al., 2003) act as BBB efflux transporters, while morphine has a saturable active influx by a yet unidentified BBB influx transporter (Groenendaal et al., 2007; Xie et al., 1999). In rats, it has been shown that blocking P-gp increases the plasma and spinal cord M6G concentrations (Lötsch et al., 2002b) while in

\* Corresponding author.

https://doi.org/10.1016/j.ejps.2023.106482

Received 21 January 2023; Received in revised form 10 May 2023; Accepted 26 May 2023 Available online 27 May 2023

0928-0987/© 2023 The Authors. Published by Elsevier B.V. This is an open access article under the CC BY license (http://creativecommons.org/licenses/by/4.0/).



E-mail address: ecmdelange@lacdr.leidenuniv.nl (E.C. de Lange).

<sup>&</sup>lt;sup>1</sup> These authors contributed equally to this work.

humans no P-gp related changes in plasma pharmacokinetics were observed (Skarke et al., 2004). The same study in humans showed that probenecid treatment decreases M6G plasma clearance, suggesting that M6G is a substrate for the probenecid-sensitive efflux transporter in the human body (Skarke et al., 2004). It has been reported that GLUT-1 and a digoxin-sensitive transporter can actively efflux M6G but with a weak capacity (Bourasset et al., 2003). For M3G, no P-gp interaction at the level of the BBB has been reported (Xie et al., 1999), while there is a possible involvement of a probenecid-sensitive efflux transporter (Xie et al., 2000). Earlier studies show the different transport mechanism involved in BBB transport of morphine and its metabolites that can influence their CNS exposure.

When considering BBB transport, constant concentrations at equilibrium (steady-state conditions) and linear pharmacokinetic relationships are often assumed. The ratio from a particular (unbound) concentration in brain and in plasma is used (i.e., a fixed  $K_{p,uu,BBB}$  value), without considering (plasma) concentration-dependency (Wright et al., 2011). The concentration-dependency should be considered for drugs with potentially nonlinear active BBB transport processes, and drugs with metabolites that compete in binding to the same receptor(s). Since morphine and its metabolites are known to be affected by nonlinear BBB transport processes, dosing schedules and/or formulations may impact the ultimately observed exposure at the target site.

The aim of this study is to evaluate the impact of nonlinear BBB transport on relative CNS exposure of morphine and its active metabolites for broad range of dosing regimens and formulations. Here we have included current clinically used morphine dosing regiments but also lower and higher ones, to explore for which dosing regimens nonlinear BBB transport matters and to evaluate whether the choice of dosing schedule or formulation could alter the impact of nonlinear transport of morphine. Here we included lower dosing regimens, as, due to the opioid crisis, the trend is to use lower morphine dosing in combination with other CNS active drugs. To that end, we will apply a physiologically based pharmacokinetic (PBPK) CNS modeling approach. This PBPK CNS model, the LeiCNS-PK3.0, predicts within two-fold error the unbound drug concentrations at different CNS compartments (Saleh et al., 2021). the LeiCNS-PK3.0 PBPK with We expand model concentration-dependent BBB transport processes of morphine. The area under the curves (AUC) and the peak-to-through ratio (PTR) for unbound plasma and unbound brain<sub>ECF</sub> pharmacokinetic profiles of morphine and its metabolites are compared to assess the effect of nonlinear BBB transport.

#### 2. Methods

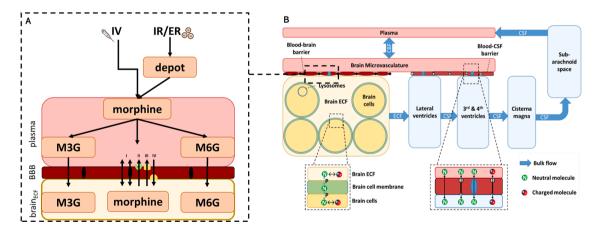
#### 2.1. Nonlinear transport blood brain barrier

The nonlinear BBB transport of unbound morphine in the LeiCNS-PK3.0 model is described by a concentration-dependent  $K_{p,uu,BBB}$  function. To derive this function, a previously published pharmacokinetic model was used that described nonlinear BBB transport of morphine in rats, which included passive diffusion, active efflux and saturable influx transport (Groenendaal et al., 2007). To obtain an equation for  $K_{p,uu,BBB}$ , this nonlinear model was simulated for rat for a wide range of doses between 0.1 and 500 mg/kg as a continuous infusion for 24 hours to obtain steady-state profiles. We then fitted a power function to relate the plasma unbound steady state concentrations to the  $K_{p,uu,BBB}$ , resulting in the following power function  $K_{p,uu,BBB} = 5.4902^{+}C_{ss,plasma}^{-0.552}$ .

#### 2.2. LeiCNS-PK3.0 PBPK model

For this study the previously published CNS PBPK model, LeiCNS-PK3.0 (Fig. 1B), was used as base model (Saleh et al., 2021). Briefly, this comprehensive model consists of a plasma and multiple CNS and cerebrospinal fluid (CSF) compartments. Between the brain microvasculature and brain<sub>ECF</sub> and CSF compartments the BBB and the blood-CSF-barrier (BSCFB) are incorporated. The multiple physiological compartments are connected through cerebral blood, brain<sub>ECF</sub> and CSF flows. Furthermore, this model takes into account pH values in each compartment, as well as brain non-specific tissue binding. As input into the LeiCNS-PK3.0 model-, on one hand, previously published human population plasma pharmacokinetic model for morphine and metabolites following IV and oral dosing was used (Fig. 1A; Table 1) (Oosten et al., 2017). The physicochemical properties of morphine and its metabolites were provided to the model (Table 1).

To describe physiological processes such as active BBB transport, the model includes asymmetry factors (AF). This value can be seen as the "pure" extent of drug distribution at the barrier, without influences of other elimination routes such as brain<sub>ECF</sub> bulk flow, which in our model are explicitly separated. The AF are calculated using  $K_{p,uu,BBB}$  values resulting in possible three situations. If  $K_{p,uu,BBB}$  is equal to 1, then the influx and efflux AF will be equal due to equilibrium of drug



**Fig. 1.** Morphine nonlinear and LeiCNS-PK3.0 model. (A) As plasma input to the LeiCNS-PK3.0 model, previously published plasma pharmacokinetic model by Oosten et al., 2017 was used. This model consisted of one compartment for morphine, morphine-3-glucuronide (M3G) and morphine-6-glucuronide (M6G) in plasma and brain extracellular fluid (brain<sub>ECF</sub>). In this model the nonlinear blood-brain barrier (BBB) transport of morphine by Groenendaal et al. is included while for the metabolites a linear transport across BBB is included. Morphine BBB transport includes I. passive para- and transcellular transport; II. efflux by P-glycoprotein III. efflux by a probenecid sensitive transporter; IV. influx by unidentified saturable influx transporter (Groenendaal et al., 2007). (B) The LeiCNS-PK3.0 model describes drug distribution in the various CNS compartments, taking into account the drug flow between different physiological compartments, various transport modes, pH influence and non-specific binding. CBF = cerebral blood flow, CNS = central nervous system, CSF= cerebrospinal fluid, ECF = extracellular fluid, *P*= octanol-water partitioning.

#### Table 1

Plasma pharmacokinetics and physical-chemical and biological properties of morphine, morphine-3-glucuronide and morphine-6-glucuronide.

	-			
		morphine	M3G	M6G
plasma PK ( Oosten et al.,	Central clearance (ml/ min)	1531.67	78.5	78.5
2017)	Central compartment volume (ml)	278,000	25,800	25,800
	Absorption rate (min <sup>-1</sup> )	IR: 0.1 ER: 0.00368	-	-
	Oral bioavailability	0.372	0.355 <sup>a</sup>	0.0631 <sup>a</sup>
	Fraction formed <sup>b</sup>	0.323	0.573	0.104
	IIV central clearance (as variance)	0.222	0.632	0.368
	IIV central compartment volume (as variance)	0.747	0.247	0.243
	Proportional residual error (as variance)	0.286	0.2	0.239
drug properties ( Wishart et al.,	Molecular weight (g/ mol)	285.34	461.46	461.46
2017)	Octanol- water lipophilicity	0.99	-0.63	0.13
	Acid ionization constant	10.26	2.67	2.87
	Base ionization constant	9.12	9.17	9.12
	Fraction unbound plasma	0.65	-	-
	fAFBBB	0.21815	1	1
	K <sub>p,uu,BBB</sub>	5.4902*C <sub>ss,u,</sub>	0.1 <sup>c</sup>	0.25 <sup>d</sup>

<sup>a</sup> fraction of metabolite formation in first-pass effect.

<sup>b</sup> fraction formed after morphine central clearance.

<sup>c</sup> obtained from Xie et al. (2000).

<sup>d</sup> obtained from Bouw et al. (2001), Tunblad et al. (2005) IIV inter individual variability.

concentration across BBB.  $K_{p,uu,BBB}$  higher than 1 suggest active efflux of drug across BBB. In this case  $AF_{efflux}$  is set to 1 and  $AF_{influx}$  is calculated. While at  $K_{p,uu,BBB}$  smaller than 1 suggest for active efflux across BBB and therefore  $AF_{efflux}$  is calculated and  $AF_{influx}$  set to 1 (the other way around for  $K_{p,uu,BBB}$  higher than 1).

In order to do simulations for humans, a human K<sub>p,uu,BBB</sub> value is needed as input. The K<sub>p,uu,BBB</sub> describing morphine nonlinear transport at BBB for human has not been determined. Therefore, the calculated rat K<sub>p,uu,BBB</sub> power function was used with a translational factor based on a transporter protein expression ratio at human versus rat BBB (abbreviated as fAFBBB) to correct the AF. This factor is only applied when a drug or metabolite is a substrate of a transporter. For morphine, two efflux (P-gp and probenecid-sensitive) and one influx transporter was taken into account. The mean protein expression level of P-gp in humans is 4.21 fmol/µg total protein (Al-Majdoub et al., 2019; Shawahna et al., 2011; Uchida et al., 2011) and in rats this is 19.28 fmol/µg total protein (Al Feteisi et al., 2018; Hoshi et al., 2013), resulting in a ratio of 0.22. For other transporters, such as the probenecid sensitive transporter and the saturable influx transporter, no expression information is available. In this case it was assumed that expression in humans and rats is equal. Since only P-gp is identified an fAFBBB of 0.22 was used for the translation of rat value of AF<sub>BBB</sub> to that of human. No data is found indicating nonlinear transport of M3G and M6G. Therefore, the K<sub>p.uu,BBB</sub> is fixed to a single value (i.e. being independent of plasma concentrations). These Kn, un BBB values are obtained from in vivo rat studies and therefore need to be translated to the humans using the fAFBBB factor. As no data on these transporters involved in metabolite transport across BBB in human is available, it was assumed that these are the same in rat and human (so the fAFBBB is fixed to 1).

#### 2.3. Simulation scenarios

Morphine and metabolite brain<sub>ECF</sub> distribution simulations for human were performed for a period of seven days in order to reach a steady state exposure. A dose range of 0.25–150 mg for intravenous (IV), oral immediate release (IR) and extended release (ER) formulations. All the doses are administered once, twice, four and six times a day. This dose range is chosen to include, beside the current clinical dosing regimens, also the doses around to investigate the impact of nonlinear BBB transport of morphine, on morphine  $\text{brain}_{ECF}$  distribution in relation to its metabolites.

#### 2.4. Evaluation of simulation scenarios

To compare the relative morphine exposure, the AUC ratio of brain  $n_{ECF}$  over plasma AUC at steady-state was used (Eq. (1)). The results are also compared for the advised clinical doses for the different formulations.

$$Relative \ exposure = \frac{AUCss, ECF}{AUCss, plasma}$$
(1)

The pharmacokinetic profile fluctuations were evaluated at day seven by comparing the peak-to-trough (PTR) calculated as in Eq. (2) (Tozer and Rowland, 2016). PTR is calculated by the highest concentration  $C_{max}$  minus lowest concentration  $C_{min}$  divided by the average concentration  $C_{av}$ .

$$PTR = \frac{Cmax, ss - Cmin, ss}{Cav, ss}$$
(2)

#### 2.5. Sensitivity analysis

A sensitivity analysis was performed for the fAFBBB parameter to evaluate the effect of variations of this parameter on the  $\text{brain}_{\text{ECF}}$  exposure (AUC<sub>ECF</sub>). Perturbations of 0.25- 2 fold changes in steps of onequarter of fAFBBB parameter was simulated.

#### 2.6. Software

Simulations for nonlinear BBB transport and LeiCNS-PK3.0 models were performed using the package RxODE version 1.1.5 and for sensitivity analysis the additional PKNCA package version 0.9.5 using R version 4.1.3.

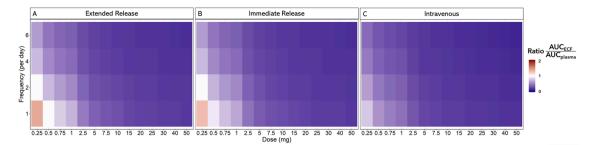
#### 3. Results

#### 3.1. Relative morphine exposure

To compare the effect of nonlinear BBB transport processes, the relative morphine exposure in the brain<sub>ECF</sub> to plasma was compared for the different formulations at steady state (day seven after treatment start). For all the administration routes, low morphine doses administrations at low frequency resulted in a relative higher exposure of unbound morphine in the brain<sub>ECF</sub> than in plasma, while increasing dose and frequency led to an increased exposure in plasma compared to brain<sub>ECF</sub> (Fig. 2). For almost all administrations, the relative morphine exposure was 1 or lower expect for ER and IR administration of 0.25 mg once-a-day. For the metabolites, no differences in relative metabolite exposure have been observed (results not shown). These results show that at low doses (<0.5 mg) and low frequency (<twice a day) administrations relative morphine exposure is higher in brain<sub>ECF</sub> than plasma.

#### 3.2. Morphine peak-to-trough ratios

To investigate the effect of nonlinear transport on the fluctuation in pharmacokinetic profiles, the PTR concentration ratios for the three



**Fig. 2.** Relative morphine exposure for different formulations and dosing schedules. For (A) oral extended release, (B) oral immediate release and (C) intravenous, the relative morphine exposure is depicted for the different frequencies per day and the dose (and milligrams) administered per time. A ratio of 1 indicates equal exposure of morphine in brain extracellular fluid (ECF) and plasma. Ratio higher than 1 indicates more exposure in brain ECF than plasma while lower than 1 indicates more exposure in plasma than in brain ECF. AUC = area under the curve.

dosing regimens were compared. The PTR versus dose in plasma was stable over the simulated dose range, while increasing the frequency, the PTR decreased as expected (Fig. 3). For  $\text{brain}_{\text{ECF}}$  there was no stable PTR versus dose range observed. The PTR increased with increasing dose and stabilized at higher doses for IV (Fig. 3), IR and ER (Supplementary Figs. S1 and S2 respectively). The  $\text{brain}_{\text{ECF}}$  PTR over the dosages shows the impact of the saturable influx transporter at lower doses resulting in a nonstable PTR over the dosages. This indicates that steady-state plasma PK profile is not representative for the  $\text{brain}_{\text{ECF}}$  PK profile.

#### 3.3. Nonlinearity effect on metabolite distribution

To study the effect on nonlinear BBB transport of morphine and its metabolites, the profiles are compared for different IV administrations at steady-state. Comparing the brain<sub>ECF</sub> peak concentrations (Cmax) of morphine to that of metabolites showed changes with increasing dose. At a low dose of 1 mg morphine, the brain<sub>ECF</sub> Cmax of morphine was higher compared to that of M3G. With increasing the dose, the M3G brain<sub>ECF</sub> Cmax increased, while the difference between the peak concentrations of morphine and those of M3G increased further (Fig. 4). For morphine versus M6G, this difference in relative C<sub>max</sub> was other way around, the difference in C<sub>max</sub> decreased with increasing dose (Fig. 4). When the metabolite to morphine exposure ratio at steady state was compared (AUCbrain<sub>ECF,metabolite</sub> /AUCbrain<sub>ECF,morphine</sub>) an increase in this exposure ratio with increasing dose was observed. For M3G/ morphine and M6G/moprhine exposure, this ratio was lower than 1 and at higher doses it increased above 1. From these results we can conclude that due to nonlinear BBB transport of morphine, the relation between morphine and metabolites brain<sub>ECF</sub> peak concentrations and brain<sub>ECF</sub>

exposure ratios changed in relation to dose changes.

#### 3.4. Sensitivity analysis

To simulate human morphine  $\mathsf{brain}_{\mathsf{ECF}}$  distribution, rat to human AF<sub>BBB</sub> factors were translated using the fAFBBB parameter. Morphine is transported by P-gp and one unidentified efflux and one unidentified influx transporter. To calculate fAFBBB to translate rat to human K<sub>p.uu</sub>. BBB values, the unidentified transporters are assumed to be equally expressed at rat and human BBB. Sensitivity analysis was performed by varying the fAFBBB value to evaluate the possible changes in the brain<sub>ECF</sub> AUC in case the human BBB transporter expression would deviate from rat values. We find that the highest impact of a change in fAFBBB would be at lower morphine doses, where the contribution of influx transport is the largest (Fig. 5). For IV administrations of once-a-day, up to 20 mg, an increase in fAFBBB would result in an increase brain<sub>ECF</sub> AUC. The opposite effect was observed for doses higher than 20 mg once a day, where an increase in fAFBBB leading to a decrease in brain<sub>ECF</sub> AUC. For IR, the possible effect of fAFBBB changes on brain<sub>ECF</sub> AUC was similar, only the shift in effects occurred at a higher dose of 70 mg once a day. For ER, this shift was even at higher dose of 110 mg once a day. The sensitivity analysis showed that the possible largest effect of fAFBBB change would be for a dose of 1 mg within the simulated range of 1 to 150 mg. For ER administrations, a decrease of 75% of fAFBBB would lead to a decrease of 65%  $\text{brain}_{\text{ECF}}$  AUC and an increase of 200% would result in an increase of 74% brain<sub>ECF</sub> AUC.

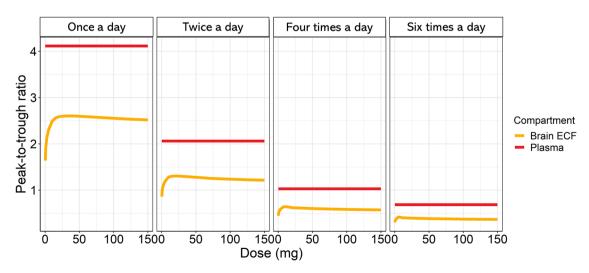
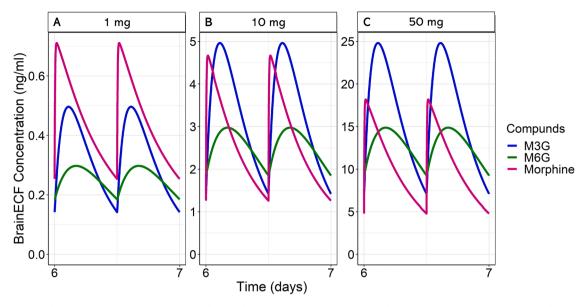
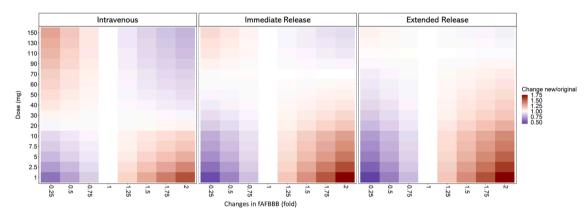


Fig. 3. Peak-to-trough ratios (PTR) of unbound morphine in plasma and brain extracellular fluid (brain<sub>ECF</sub>), as a function of the dose. PTR in plasma and brain<sub>ECF</sub> after IV administration of once, twice, and six times a day.



**Fig. 4.** Morphine, morphine-3-glucuronide (M3G) and morphine-6-glucuronide (M6G) distribution in brain extracellular fluid (brain<sub>ECF</sub>) following different dose regimens. The concentration over time profiles of morphine and its metabolites at the brain<sub>ECF</sub> for 1 (A), 10 (B) and 50 (C) mg twice day IV administration of morphine is compared at steady state (day seven).



**Fig. 5.** Sensitivity analysis for expression of transporters effect on AUC brain extracellular fluid (brain<sub>ECF</sub>) for different dosing regimens. Sensitivity analysis for differences in factor asymmetry factor at blood brain barrier (fAFBBB) and impact on the brain<sub>ECF</sub> AUC for different doses (1 to 150 mg), perturbations (0.25–2-fold changes) and formulations (intravenous, oral immediate and oral extended administrations). Blue indicates a lower new brain<sub>ECF</sub> AUC compared to original value, white indicates no changes and red a higher new value.

#### 4. Discussion

In this study we evaluated the impact of nonlinear BBB transport on distribution of morphine and its active metabolites in the brain<sub>ECF</sub>, by expanding the LeiCNS-PK3.0 PBPK model with nonlinear BBB transport processes. We showed that nonlinear BBB transport of morphine affects the relative target site exposure and PTR, as well as the relation of morphine to its metabolite brain<sub>ECF</sub> exposure mainly at low doses.

Our model predicts the importance of including nonlinear BBB transport to evaluate human  $\text{brain}_{\text{ECF}}$  concentration of morphine and its metabolites. For ethical reasons no such direct information can be obtained from human. Due to the lack of such knowledge in humans an inherent uncertainty exists for the human morphine  $\text{brain}_{\text{ECF}}$  predictions with assumptions dependent on the availability of data. In this study, nonlinear BBB transport was implemented for predicting morphine brain<sub>ECF</sub> pharmacokinetics, based on previous *in vivo* mice and rat studies that provided quantitative information on plasma concentration dependent BBB influx transport and non-saturable BBB efflux transport processes (Groenendaal et al., 2007; Xie et al., 1999). The extended LeiCNS-PK3.0 model (Saleh et al., 2021; Yamamoto et al., 2017a,

2017b) needs as input a plasma concentration-dependent human  $K_{p,uu}$ , BBB (nonlinear BBB transport) of morphine, but such data are not available in human. So, rat values for concentration-dependent  $K_{p,uu,BBB}$ values were derived (Groenendaal et al., 2007), and used in combination with rat to human transporter expression translational factor, fAFBBB, to correct the AF<sub>BBB</sub>. Here the fAFBBB is the relative expression factor of transporters on the BBB in rat and human (Al-Majdoub et al., 2019; Shawahna et al., 2011; Uchida et al., 2011; Yamamoto et al., 2018). Transporters at BBB play a crucial role in drug exposure at brain<sub>ECF</sub>. For this reason, using the relative expression factor as translational factor from rat to human is useful (Yamamoto et al., 2018).

We assumed both unidentified transporters for morphine BBB influx and efflux are equally expressed in rat and human, while the expression of P-gp was scaled from rat to human based on available relative expression values (Al-Majdoub et al., 2019; Shawahna et al., 2011; Uchida et al., 2011; Yamamoto et al., 2018). The sensitivity analysis has shown the possible impact of changes in the fAFBBB on the brain<sub>ECF</sub> exposure. The results indicate the importance of identification of these transporters, mainly at lower doses where morphine brain<sub>ECF</sub> exposure is mostly affected by changes in fAFBBB. For morphine transport across the BBB, P-gp is the only identified active transporter. Another efflux transporter is probenecid dependent as best current knowledge, and furthermore, there is an unidentified saturable influx transporter. Probenecid is known to be an inhibitor for many transporters including multidrug resistance associated proteins (MRPs). The organic anion transporter 1 and 3 (oat1, oat3) and organic anion transporting polypeptide 1 and 2 (oatp1, oatp2) are also inhibited by probenecid (Sugivama et al., 2001). The possible influx transporter could be the organic cationic transporter 1 (OCT1). Previous study have shown that OCT1 plays а role in hepatocellular saturable and concentration-dependent uptake of morphine (Tzvetkov et al., 2013) and for some cationic compounds in rat and human transfected hepatocytes (Umehara et al., 2007). Whether these suggested transporters are involved in morphine transport their presence at human BBB and transport of morphine should be confirmed. Another possible influx transporter involved could be the pyrilamine transporter. In an *in vitro* BBB model oxycodone transport via the pyrilamine transporter was examined alone and in combination with other compounds among other as morphine. The results showed that morphine can inhibit oxycodone uptake suggesting the possibility of morphine being a substrate for an BBB influx transporter (Okura et al., 2008).

The impact of every transporter on the transport of morphine across BBB,  $K_{p,uu,BBB}$ , can roughly be estimated based on previous *in vivo* studies comparing the  $K_{p,uu,BBB}$  in transporter inhibited conditions. In an *in vivo* study where P-gp was blocked by administration of GF120918, morphine  $K_{p,uu,BBB}$  increased from 0.47 to 1.21, a significant increase of  $\pm$  2.5-fold (Letrent et al., 1999). From an *in vivo* study with probenecid administration, the results showed an increase of  $K_{p,uu,BBB}$  from 0.29 to 0.39 indicating an increase of  $\pm$  1.3-fold (Tunblad et al., 2003). These results shows that the total impact of P-gp is possibly higher compared to the probenecid-sensitive transporter. The two efflux transporter are assumed to behave linearly over plasma concentration. This would mean that the saturable influx transporter has the major impact on transport of morphine across BBB at lower plasma concentrations ( $K_{p,uu,BBB} > 1$ ) and its impact is decreasing over increasing plasma concentration.

The factor used to translate between rat and human BBB transporter expression (fAFBBB) was set to a value of 1 for transporters other than Pgp. This is to remain on the safe side as there is no clear information on transporters other than P-gp involved in the morphine and/or metabolite BBB transport in human. Specifically; the probenecid-sensitive transporter seems to play a role in M3G and morphine active BBB efflux transport in rats (Tunblad et al., 2003; Xie et al., 2000) but not for M6G while for M6G a  $K_{p,uu,BBB}$  value of 0.3 was found, indicating active BBB efflux of M6G, but not by the probenecid-sensitive transporters (Tunblad et al., 2005), while it is unclear if M6G is a weak (if at all) P-gp substrate (Lötsch et al., 2002a). Bourasset et al. (2003) indicated that M6G is not a P-gp substrate but merely a weak substrate for GLUT-1 and a digoxin-sensitive transporter. These studies indicated there is still a knowledge gap on the exact transporters being involved in the BBB transport of the metabolites. Therefore, we displayed the scenario that K<sub>p.uu.BBB</sub> values found for the metabolites in rats would be the same as those in human.

This study has shown that nonlinear BBB transport mainly affects morphine brain<sub>ECF</sub> pharmacokinetics at lower dose and lower dosing frequencies for IV, oral IR and ER formulations. With increasing dose, the influx BBB transport of morphine becomes saturated, and its BBB transport becomes mostly linear with plasma concentrations. This nonlinear BBB transport effect is outside the clinical dosing regimens for adults (FDA, 2012, 1984), suggesting no direct impact of nonlinear BBB transport on morphine treatment to adults. The effect of nonlinear BBB of morphine in the lower dosing regimens (than currently used for adults) is of special interest, as the trend is to lower opioid use by combining with other CNS active drugs. The aim is here to have good (/improved) analgesia, but to have lower abuse liability, sedation and cognitive impairment. Then, for pediatrics, nonlinear BBB transport might have more impact on the treatment regimens. Clinical dosing regimens of morphine in pediatrics mainly is calculated based on their weights resulting for example in oral regimens for pediatrics younger than 12 years a maximum of 200–500 mcg/kg every 4 hours with a maximum of 5 mg per day (Unknown author, 2012). With this, the total dose of morphine in pediatrics can be at the dose where the saturable influx transporter has more impact and may lead to a morphine brain<sub>ECF</sub> exposure that is relatively higher which may have an influence on the effect as well as side effects. This may be point of consideration for morphine dosing in pediatric patients.

To our best knowledge, nonlinear BBB transport is applicable for morphine, but not for M3G and M6G. The effect of nonlinear BBB transport on the relation of morphine with its metabolites at  $\text{brain}_{\text{ECF}}$  has not been studied before. We found that increasing plasma concentrations result in different brain<sub>ECF</sub> concentrations ratios of M3G/morphine and M6G/morphine. This may have an impact on their relative receptor binding. The target receptors of morphine and its metabolites are the mu1, mu2, delta and kappa opioid receptors (Imming et al., 2007; Kristensen, 1995). These receptors are predominantly present in the CNS (Peng et al., 2012). For morphine and M6G to exerts their analgesic effect, they should bind to the mu-opioid receptors (Rainville, 2002; Vanderah, 2010; Yamada et al., 2006) and therefore compete with each other. M3G, on the other hand, has a low potency for the mu-opioid receptor (Frölich et al., 2011). In humans, it has been debated that M3G can cause hyperalgesia by binding to Toll-like receptor 4 and may lead to cross-talk of the Toll-like receptor 4 and mu-opioid receptor (Gabel et al., 2022). By binding to the mu-opioid and Toll-like receptors, morphine and M6G actives the  $G_i$ -protein and  $\beta$ -arrestin while M3G has a lower potency and activates scaffold proteins (Frölich et al., 2011; Gabel et al., 2022). The sensitivity analysis has provided the possible effects of a different fAFBBB on brain<sub>ECF</sub> exposure between rat and human. The results showed that the  $\mathsf{brain}_{\mathsf{ECF}}$  exposure changes mainly at lower morphine doses. Such changes in brain<sub>ECF</sub> exposure can lead to changes in relation of morphine with is metabolites and with that the possible interaction at the mu-opioid receptors. Altogether, this indicates the need for understanding brain<sub>ECF</sub> exposure as step one, followed by further exploration on the consequences on receptor binding.

One aspect not yet taken into account in this study is the possible metabolism of morphine within the CNS. This study assumed only metabolism of morphine in the liver and used plasma pharmacokinetics with fixed metabolite fractions (Oosten et al., 2017). However, a previous study has shown possible M6G formation from morphine in human brain homogenates (Yamada et al., 2003), and also in rat microglia (Togna et al., 2013). This needs to be further investigated.

#### 5. Conclusion

In conclusion, our simulations indicate that nonlinear BBB transport of morphine and its metabolites may affect exposure in  $\text{brain}_{\text{ECF}}$  target site concentrations, in particular at lower doses, enabled by an in silico PBPK modeling approach using the LeiCNS-PK3.0 model.

#### Funding

This project has received funding from the European Union's Horizon 2020 research and innovation program under grant agreement No 848068. This manuscript reflects only the authors' view and the European Commission is not responsible for any use that may be made of the information it contains.

#### Credit author statement

Berfin Gülave: Conceptualization, Data collection, preparation and analysis, Model simulations, Writing original draft, review and editing.

Divakar Budda: Conceptualization, Data collection, preparation and analysis, Model simulations, Writing original draft, review and editing. Mohammed AA Saleh: Data preparation and analysis. JG Coen van Hasselt: Conceptualization, Writing original draft, review and editing.

**Elizabeth CM de Lange:** Conceptualization, Writing original draft, review and editing.

#### **Declaration of Competing Interest**

NA

#### Data availability

No data was used for the research described in the article.

#### Supplementary materials

Supplementary material associated with this article can be found, in the online version, at doi:10.1016/j.ejps.2023.106482.

#### References

- Al-Majdoub, Z.M., Al Feteisi, H., Achour, B., Warwood, S., Neuhoff, S., Rostami-Hodjegan, A., Barber, J., 2019. Proteomic quantification of human blood-brain barrier SLC and ABC transporters in healthy individuals and dementia patients. Mol. Pharm. 16, 1220–1233. https://doi.org/10.1021/acs.molpharmaceut.8b01189.
- Al Feteisi, H., Al-Majdoub, Z.M., Achour, B., Couto, N., Rostami-Hodjegan, A., Barber, J., 2018. Identification and quantification of blood–brain barrier transporters in isolated rat brain microvessels. J. Neurochem. 146, 670–685. https://doi.org/ 10.1111/jnc.14446.
- Bourasset, F., Cisternino, S., Temsamani, J., Scherrmann, J.M., 2003. Evidence for an active transport of morphine-6-β-D-glucuronide but not P-glycoprotein-mediated at the blood-brain barrier. J. Neurochem. 86, 1564–1567. https://doi.org/10.1046/ j.1471-4159.2003.01990.x.
- Bouw, M.R., Xie, R., Tunblad, K., Hammarlund-Udenaes, M., 2001. Blood-brain barrier transport and brain distribution of morphine-6-glucuronide in relation to the antinociceptive effect in rats - Pharmacokinetic/pharmacodynamic modelling. Br. J. Pharmacol. 134, 1796–1804. https://doi.org/10.1038/sj.bjp.0704406.
- Chaves, C., Remiao, F., Cisternino, S., Decleves, X., 2017. Opioids and the blood-brain barrier: a dynamic interaction with consequences on drug disposition in brain. Curr. Neuropharmacol. 15, 1156–1173. https://doi.org/10.2174/ 1570159x15666170504095823.

Christrup, L.L., 1997. Morphine metabolites. Acta Anaesthesiol. Scand. 41, 116–122. https://doi.org/10.1111/j.1399-6576.1997.tb04625.x.

- De Gregori, S., De Gregori, M., Ranzani, G.N., Allegri, M., Minella, C., Regazzi, M., 2012. Morphine metabolism, transport and Brain disposition. Metab. Brain Dis. 27, 1–5. https://doi.org/10.1007/s11011-011-9274-6.
- FDA, 2012. Morphine sulphate tablets FDA label. Ref. ID 3075779.

FDA, 1984. Morphine sulfate injection FDA label.

- Frölich, N., Dees, C., Paetz, C., Ren, X., Lohse, M.J., Nikolaev, V.O., Zenk, M.H., 2011. Distinct pharmacological properties of morphine metabolites at G i-protein and β-arrestin signaling pathways activated by the human μ-opioid receptor. Biochem. Pharmacol. 81, 1248–1254. https://doi.org/10.1016/j.bcp.2011.03.001.
- Gabel, F., Hovhannisyan, V., Berkati, A.K., Goumon, Y., 2022. Morphine-3-Glucuronide, Physiology and Behavior. Front. Mol. Neurosci. 15, 1–16. https://doi.org/10.3389/ fnmol.2022.882443.
- Groenendaal, D., Freijer, J., De Mik, D., Bouw, M.R., Danhof, M., De Lange, E.C.M., 2007. Population pharmacokinetic modelling of non-linear brain distribution of morphine: influence of active saturable influx and P-glycoprotein mediated efflux. Br. J. Pharmacol. 151, 701–712. https://doi.org/10.1038/sj.bjp.0707257.
- Hoshi, Y., Uchida, Y., Tachikawa, M., Inoue, T., Ohtsuki, S., Terasaki, T., 2013. Quantitative atlas of blood–brain barrier transporters, receptors, and tight junction proteins in rats and common marmoset. J. Pharm. Sci. 102, 3343–3355. https://doi. org/10.1002/jps.23575.
- Imming, P., Sinning, C., Meyer, A., 2007. Drugs, their targets and the nature and number of drug targets 5, 821–835.
- Klimas, R., Mikus, G., 2014. Morphine-6-glucuronide is responsible for the analgesic effect after morphine administration: a quantitative review of morphine, morphine-6-glucuronide, and morphine-3-glucuronide. Br. J. Anaesth. 113, 935–944. https:// doi.org/10.1093/bja/aeu186.
- Kristensen, K., 1995. The mu1, mu2, delta, kappa opioid receptor binding profiles of methadone stereoisomers and morphine. Life Sci. 56, PL45–PL50. https://doi.org/ 10.1016/0024-3205(94)00426-S.
- Letrent, S.P., Pollack, G.M., Brouwer, K.R., Brouwer, K.L.R., 1999. Effects of a potent and specific P-glycoprotein inhibitor on the blood- brain barrier distribution and antinoclceptive effect of morphine in the rat. Drug Metab. Dispos. 27, 827–834.
- Lötsch, J., Schmidt, R., Vetter, G., Schmidt, H., Niederberger, E., Geisslinger, G., Tegeder, I., 2002a. Increased CNS uptake and enhanced antinociception of morphine-6-glucuronide in rats after inhibition of P-glycoprotein. J. Neurochem. 83, 241–248. https://doi.org/10.1046/j.1471-4159.2002.01177.x.

- Lötsch, J., Skarke, C., Schmidt, H., Liefhold, J., Geisslinger, G., 2002b. Pharmacokinetic modeling to predict morphine and morphine-6-glucuronide plasma concentrations in healthy young volunteers. Clin. Pharmacol. Ther. 72, 151–162. https://doi.org/ 10.1067/mcp.2002.126172.
- Murthy, B.P., Pollack, G.M., Brouwer, K.L.R., 2002. Contribution of morphine-6glucuronide to antinociception following intravenous administration of morphine to healthy volunteers. J. Clin. Pharmacol. 42, 569–576. https://doi.org/10.1177/ 00912700222011508.
- Okura, T., Hattori, A., Takano, Y., Sato, T., Hammarlund-Udenaes, M., Terasaki, T., Deguchi, Y., 2008. Involvement of the pyrilamine transporter, a putative organic cation transporter, in blood-brain barrier transport of oxycodone. Drug Metab. Dispos. 36, 2005–2013. https://doi.org/10.1124/dmd.108.022087.
- Oosten, A.W., Abrantes, J.A., Jönsson, S., Matic, M., van Schaik, R.H.N., de Bruijn, P., van der Rijt, C.C.D., Mathijssen, R.H.J., 2017. A prospective population pharmacokinetic study on morphine metabolism in cancer patients. Clin. Pharmacokinet. 56, 733–746. https://doi.org/10.1007/s40262-016-0471-7.
- Peng, J., Sarkar, S., Chang, S.L., 2012. Opioid receptor expression in human brain and peripheral tissues using absolute quantitative real-time RT-PCR. Drug Alcohol Depend. 124, 223–228. https://doi.org/10.1016/j.drugalcdep.2012.01.013.
- Rainville, P., 2002. Brain mechanisms of pain affect and pain modulation. Curr. Opin. Neurobiol. 12, 195–204. https://doi.org/10.1016/S0959-4388(02)00313-6.
- Saleh, M.A.A., Loo, C.F., Elassaiss-Schaap, J., De Lange, E.C.M., 2021. Lumbar cerebrospinal fluid-to-brain extracellular fluid surrogacy is context-specific: insights from LeiCNS-PK3.0 simulations. J. Pharmacokinet. Pharmacodyn. 48, 725–741. https://doi.org/10.1007/s10928-021-09768-7.
- Shawahna, R., Uchida, Y., Declèves, X., Ohtsuki, S., Yousif, S., Dauchy, S., Jacob, A., Chassoux, F., Daumas-Duport, C., Couraud, P.O., Terasaki, T., Scherrmann, J.M., 2011. Transcriptomic and quantitative proteomic analysis of transporters and drug metabolizing enzymes in freshly isolated human brain microvessels. Mol. Pharm. 8, 1332–1341. https://doi.org/10.1021/mp200129p.
- Skarke, C., Langer, M., Jarrar, M., Schmidt, H., Geisslinger, G., Lötsch, J., 2004. Probenecid interacts with the pharmacokinetics of morphine-6-glucuromide in humans. Anesthesiology 101, 1394–1399. https://doi.org/10.1097/00000542-200412000-00020.
- Sugiyama, D., Kusuhara, H., Shitara, Y., Abe, T., Meier, P.J., Sekine, T., Endou, H., Suzuki, H., Sugiyama, Y., 2001. Characterization of the efflux transport of 17βestradiol-D-17β-glucuronide from the brain across the blood-brain barrier. J. Pharmacol. Exp. Ther. 298, 316–322.
- Togna, A.R., Antonilli, L., Dovizio, M., Salemme, A., De Carolis, L., Togna, G.I., Patrignani, P., Nencini, P., 2013. *In vitro* morphine metabolism by rat microglia. Neuropharmacology 75, 391–398. https://doi.org/10.1016/j. neuropharm.2013.08.019.
- Tozer, T.B., Rowland, M., 2016. Essentials of Pharmacokinetics and Pharmacodynamics. Wolters Kluwer.
- Tunblad, K., Hammarlund-Udenaes, M., Jonsson, E.N., 2005. Influence of probenecid on the delivery of morphine-6-glucuronide to the brain. Eur. J. Pharm. Sci. 24, 49–57. https://doi.org/10.1016/j.ejps.2004.09.009.
- Tunblad, K., Jonsson, E.N., Hammarlund-Udenaes, M., 2003. Morphine blood-brain barrier transport is influenced by probenecid co-administration. Pharm. Res. 20, 618–623. https://doi.org/10.1023/A:1023250900462.
- Tzvetkov, M.V., Dos Santos Pereira, J.N., Meineke, I., Saadatmand, A.R., Stingl, J.C., Brockmöller, J., 2013. Morphine is a substrate of the organic cation transporter OCT1 and polymorphisms in OCT1 gene affect morphine pharmacokinetics after codeine administration. Biochem. Pharmacol. 86, 666–678. https://doi.org/ 10.1016/j.bcp.2013.06.019.
- Uchida, Y., Ohtsuki, S., Katsukura, Y., Ikeda, C., Suzuki, T., Kamile, J., Terasaki, T., 2011. Quantitative targeted absolute proteomics of human blood-brain barrier transporters and receptors. J. Neurochem. 117, 333–345. https://doi.org/10.1111/j.1471-4159.2011.07208.x.
- Umehara, K.I., Iwatsubo, T., Noguchi, K., Kamimura, H., 2007. Functional involvement of organic cation transporter1 (OCT1/Oct1) in the hepatic uptake of organic cations in humans and rats. Xenobiotica 37, 818–831. https://doi.org/10.1080/ 00498250701546012.

Unknown author, 2012. Essential medicines: paediatric morphine dosage. WHO Drug Inf. 26, 278–281.

- Vanderah, T.W., 2010. Delta and kappa opioid receptors as suitable drug targets for pain. Clin. J. Pain 26, 10–15. https://doi.org/10.1097/AJP.0b013e3181c49e3a.
- Wishart, D.S., Feunang, Y.D., Guo, A.C., Lo, E.J., Marcu, A., Grant, J.R., Sajed, T., Johnson, D., Li, C., Sayeeda, Z., Iynkkaran, N.A.I., Liu, Y., Maciejewski, A., Gale, N., AlexWilson, Chin, L., Cummings, R., Le, D., Pon, A., Knox, C., Wilson, M., 2017. DrugBank 5.0: a major update to the DrugBank database for 2018. Nucleic Acids Res. 46, D1074–D1082. https://doi.org/10.1093/nar/gkx1037.
- Wright, D.F.B., Winter, H.R., Duffull, S.B., 2011. Understanding the time course of pharmacological effect: a PKPD approach. Br. J. Clin. Pharmacol. 71, 815–823. https://doi.org/10.1111/j.1365-2125.2011.03925.x.
- Xie, R., Bouw, M.R., Hammarlund-Udenaes, M., 2000. Modelling of the blood-brain barrier transport of morphine-3-glucuronide studied using microdialysis in the rat: involvement of probenecid-sensitive transport. Br. J. Pharmacol. 131, 1784–1792. https://doi.org/10.1038/sj.bjp.0703759.
- Xie, R., Hammarlund-Udenaes, M., De Boer, A.G., De Lange, E.C.M., 1999. The role of Pglycoprotein in blood-brain barrier transport of morphine: transcortical microdialysis studies in mdr1a (-/-)and mdr1a (+/+) mice. Br. J. Pharmacol. 128, 563–568. https://doi.org/10.1038/sj.bjp.0702804.
- Yamada, H., Ishii, K., Ishii, Y., Ieiri, I., Nishio, S., Morioka, T., Oguri, K., 2003. Formation of highly analgesic morphine-6-glucuronide following physiologic concentration of

B. Gülave et al.

morphine in human brain. J. Toxicol. Sci. 28, 395–401. https://doi.org/10.2131/jts.28.395.

- Yamada, H., Shimoyama, N., Sora, I., Uhl, G.R., Fukuda, Y., Moriya, H., Shimoyama, M., 2006. Morphine can produce analgesia via spinal kappa opioid receptors in the absence of mu opioid receptors. Brain Res. 1083, 61–69. https://doi.org/10.1016/j. brainres.2006.01.095.
- Yamamoto, Y., Välitalo, P.A., Huntjens, D.R., Proost, J.H., Vermeulen, A., Krauwinkel, W., Beukers, M.W., Van Den Berg, D.J., Hartman, R., Wong, Y.C., Danhof, M., Van Hasselt, J.G.C., De Lange, E.C.M., 2017a. Predicting drug concentration-time profiles in multiple CNS compartments using a comprehensive physiologically-based pharmacokinetic model. CPT Pharmacomet. Syst. Pharmacol. 6, 765–777. https://doi.org/10.1002/psp4.12250.
- Yamamoto, Y., Välitalo, P.A., van den Berg, D.J., Hartman, R., van den Brink, W., Wong, Y.C., Huntjens, D.R., Proost, J.H., Vermeulen, A., Krauwinkel, W., Bakshi, S., Aranzana-Climent, V., Marchand, S., Dahyot-Fizelier, C., Couet, W., Danhof, M., van Hasselt, J.G.C., de Lange, E.C.M., 2017b. A generic multi-compartmental CNS distribution model structure for 9 drugs allows prediction of human brain target site concentrations. Pharm. Res. 34, 333–351. https://doi.org/10.1007/s11095-016-2065-3.
- Yamamoto, Y., Välitalo, P.A., Wong, Y.C., Huntjens, D.R., Proost, J.H., Vermeulen, A., Krauwinkel, W., Beukers, M.W., Kokki, H., Kokki, M., Danhof, M., van Hasselt, J.G. C., de Lange, E.C.M., 2018. Prediction of human CNS pharmacokinetics using a physiologically-based pharmacokinetic modeling approach. Eur. J. Pharm. Sci. 112, 168–179. https://doi.org/10.1016/j.ejps.2017.11.011.