SHORT COMMUNICATION



Automated image registration of cerebral digital subtraction angiography

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Abstract

Purpose Our aim is to automatically align digital subtraction angiography (DSA) series, recorded before and after endovascular thrombectomy. Such alignment may enable quantification of procedural success.

Methods Firstly, we examine the inherent limitations for image registration, caused by the projective characteristics of DSA imaging, in a representative set of image pairs from thrombectomy procedures. Secondly, we develop and assess various image registration methods (SIFT, ORB). We assess these methods using manually annotated point correspondences for thrombectomy image pairs.

Results Linear transformations that account for scale differences are effective in aligning DSA sequences. Two anatomical landmarks can be reliably identified for registration using a U-net. Point-based registration using SIFT and ORB proves to be most effective for DSA registration and are applicable to recordings for all patient sub-types. Image-based techniques are less effective and did not refine the results of the best point-based registration method.

Conclusion We developed and assessed an automated image registration approach for cerebral DSA sequences, recorded before and after endovascular thrombectomy. Accurate results were obtained for approximately 85% of our image pairs.

Keywords Digital subtraction angiography · Ischemic stroke · Endovascular thrombectomy · Image registration

Introduction

Ischemic stroke is the most common type of stroke (71%), a leading cause of disability and death [1]. Endovascular thrombectomy (EVT) aims to restore blood flow by mechanical removal of the thrombus. Intermittently, digital subtraction angiography (DSA) is used to visualize and study [2] the vessels.

A quantitative comparison of the vessels (or perfusion) before and after the intervention may lead to a better understanding of the result of the intervention and may also permit prediction of outcome [3, 4]. Such a comparison of DSA series is currently hampered by the lack of an accurate spa-

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² Maastricht University Medical Center, Maastricht, The Netherlands tial alignment [5] for series obtained before and after the treatment.

Automating such alignment is challenging, as there may be new arteries visualized after a (partially) successful thrombus removal. Additionally, spatial correspondence likely requires a nonlinear deformation, even for subsequent frames, as is indicated by early work [6] on DSA image processing. Finally, the orientation of the imaging setup, with respect to the patient, can vary significantly during a procedure, as the ischemic stroke patient will move during the procedure. Additionally, the radiologist changes the orientation intermittently for anterior–posterior (AP) or lateral views.

In this work, we aim to develop and assess an image registration strategy on a large set of images using a quantitative metric. We will first investigate which type of transformation is effective in aligning different DSA series. Subsequently, traditional registration methods and a deep learning method are adapted and assessed for automated alignment.

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Fig. 1 DSA images of an ischemic stroke patient, including annotated point-correspondences for pre-/post-EVT (red/blue) minIPs for AP and lateral views (left/right)



Fig. 2 Average residual error distributions of optimized transformations for AP image pairs

Methods

The effects of patient movement and differences in C-arm orientation, inherently present in DSA data, may require additional transformation complexity for effective alignment. Ultimately, it is not apparent what transformation type is suitable to model the projection of 3D motion. We therefore empirically investigate what transformation type is suited for spatial alignment by fitting different 2D transformations to manually annotated point correspondences.

Subsequently, we assess automatic registration techniques. We first develop a neural network to identify two cerebral artery landmarks, which will provide point correspondences for all DSA sequences. For more accurate alignment of sequences pre- and post-EVT images of the same patient, point correspondences from traditional methods, SIFT (scale-invariant feature transform) [7] and ORB (Oriented FAST and Rotated BRIEF) [8], are used.

The neural network uses the U-net architecture [9] to compute the probability distributions of the location of the two landmarks (see Fig. 3). The final sigmoid activation function enforces the lower and upper bounds of the probability values. At inference, the landmark positions are determined by the highest probability (argmax) or expectation (centre of mass). Kullback–Leibler (KL) divergence [10] and Jensen– Shannon (JS) divergence [11] are used as loss functions w.r.t Gaussian distributions centred on manual annotations.

Data

In this work, we use imaging data from the MR CLEAN Registry [12], a registry of consecutive stroke patients treated with EVT in the Netherlands. An initial selection of preand post-EVT sequences from the MR CLEAN Registry is adopted from a previous study [4]. A subsequent selection is done to reduce annotation time while retaining a representative view of clinical variability. This resulted in 104 patients to be included, of which the pre-/post-EVT AP and lateral DSA series are evaluated. Figure 1 is one such patient record. During the U-net model training and validation, procedural recordings of other patients were used: 1716 AP and 1472 lateral series in total.

Experiments and results

Intra-patient manual transformation assessment

To assess the impact of additional degrees of freedom on alignment accuracy, global transformations are optimized for manually annotated pre- and post-EVT recordings of 104 patients. Image pairs with fewer than six point correspondences are excluded to prevent overfitting. The resulting error distributions per transformation type are shown in Fig. 2.



Fig. 3 ICA and M1 landmark predictions for A AP and B lateral MinIPs. C AP landmark prediction error distributions for the three data splits for the best-performing configuration

Landmark detection

For the assessment of the U-net-based landmark detection, we performed a threefold cross-validation. In this crossvalidation, the data are randomly split based on patient id, thereby preventing validation and training on images from the same patient. Models were trained using different loss functions and the Adam optimizer until convergence was achieved. Weights were saved for the epoch with the best centre-of-mass prediction error on the validation set. The results are shown in Fig. 3.

Point-based registration

We examined transformations computed with automatically identified point-correspondences using the landmark model, SIFT, and ORB. The success rate of finding sufficient inliers (≥ 5) for combinations of these methods is summarised in Table 1.

Accuracy distributions of the methods, excluding the invalid solutions, are shown in Fig. 4. The range of the registration error is equivalent to Fig. 2. Each distribution represents a different image subset, i.e. the valid solutions of the method. For an unbiased method comparison, see Appendix B.7.

Discussion and conclusion

We have investigated approaches to automatically align cerebral DSA series. Transformations that account for differences in scale are capable of aligning cerebral DSA sequences. Transformations with additional degrees of freedom are

Table [•]	Number of so	olutions (TP+FP) and invalid solut	tions (FP) found
using	automatically i	identified point	correspondences	for 104 image
pairs				

Methods			AP		Lateral	
SIFT	ORB	LM	TP+FP	FP	TP+FP	FP
\checkmark	×	×	58	0	65	2
×	\checkmark	×	101	23	103	21
\checkmark	\checkmark	×	101	19	104	16
\checkmark	×	\checkmark	67	1	76	1
×	\checkmark	\checkmark	102	23	104	19
\checkmark	\checkmark	\checkmark	101	20	103	16

Bold values indicate the solution with most successful registrations Solutions with an average error greater than 10px are classified as invalid, based on Fig. 2

marginally more accurate. Although this could be attributed to improved modelling of projection of 3D motion, it is more likely a consequence of overfitting.

A deep-learning strategy using the U-net architecture proved capable of identifying cerebral artery landmarks to 4px accuracy. Performing image registration using the two landmarks proved limited, only yielding improved translation. Automatic image registration of pre-/post-EVT DSA sequences can, however, be performed using traditional point-based methods. SIFT produces negligible outliers with a lower success rate than ORB, which finds more solutions (+40%) at the cost of an increased false discovery rate (+20%). The accuracy of the point-based methods approaches the residual alignment error of manual annotations.

Combined, an 85% success rate is achieved with comparable performance for various types of stroke patients and



Fig.4 Registration error for least-squares similarity transformations using automatically identified point correspondences for lateral DSA images

procedural outcomes. This will enable further automation of DSA image analysis and procedure evaluation, contributing to outcome prediction and procedural decision-making for EVT.

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Declarations

Conflict of interest The authors declare that they have no conflict of interest.

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References

- 1. WHO (2020) WHO methods and data sources for country-level causes of death 2000–2019. Global Health Estimates Technical Paper
- Dargazanli C, Consoli A, Barral M, Labreuche J, Redjem H, Ciccio G et al (2017) Impact of modified TICI 3 versus modified TICI 2b reperfusion score to predict good outcome following endovascular therapy. Am J Neuroradiol. https://doi.org/10.3174/ajnr.A4968

- Prasetya H, Ramos LA, Epema T, Treurniet KM, Emmer BJ, Van Den Wijngaard IR et al (2021) qTICI: quantitative assessment of brain tissue reperfusion on digital subtraction angiograms of acute ischemic stroke patients. Int J Stroke 16(2):207–216
- 4. Su R, Cornelissen SA, Van Der Sluijs M, Van Es AC, Van Zwam WH, Dippel DW et al (2021) autoTICI: automatic brain tissue reperfusion scoring on 2D DSA images of acute ischemic stroke patients. IEEE Trans Med Imaging 40(9):2380–2391
- Liebeskind A, Deshpande A, Murakami J, Scalzo F (2019) Automatic estimation of arterial input function in digital subtraction angiography. In: Advances in visual computing: 14th international symposium on visual computing, ISVC 2019, Lake Tahoe, NV, USA, October 7–9, 2019, Proceedings, Part I. Springer, pp 393–402
- Meijering EH, Niessen WJ, Bakker J, Van Der Molen AJ, de Kort GA, Lo RT et al (2001) Reduction of patient motion artifacts in digital subtraction angiography: evaluation of a fast and fully automatic technique. Radiology 219(1):288–293
- Lowe DG (2004) Distinctive image features from scale-invariant keypoints. Int J Comput Vis 60(2):91–110
- Rublee E, Rabaud V, Konolige K, Bradski G (2011) ORB: an efficient alternative to SIFT or SURF. In: 2011 International conference on computer vision. IEEE, pp 2564–2571
- Ronneberger O, Fischer P, Brox T (2015) U-net: convolutional networks for biomedical image segmentation. In: International conference on medical image computing and computer-assisted intervention. Springer, pp 234–241
- Kullback S, Leibler RA (1951) On information and sufficiency. Ann Math Stat. https://doi.org/10.1214/aoms/1177729694
- Lin J (1991) Divergence measures based on the Shannon entropy. IEEE Trans Inf Theory. https://doi.org/10.1109/18.61115
- Jansen IGH, Mulder MJHL, Goldhoorn RB, MR CLEAN Registry Investigators (2018) Endovascular treatment for acute ischaemic stroke in routine clinical practice: prospective, observational cohort study (MR CLEAN Registry). BMJ 360:k949. https://doi.org/10. 1136/bmj.k949

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