



Analyst

Accepted Manuscript

This article can be cited before page numbers have been issued, to do this please use: V. Manoharan, R. Rodrigues, S. Sadati, M. J. Swann, N. Freeman, B. Du, E. Yildirim, U. Tamer, T. N. Arvanitis, D. Isakov, A. Asadipour and J. Charmet, *Analyst*, 2023, DOI: 10.1039/D2AN01350A.



This is an Accepted Manuscript, which has been through the Royal Society of Chemistry peer review process and has been accepted for publication.

Accepted Manuscripts are published online shortly after acceptance, before technical editing, formatting and proof reading. Using this free service, authors can make their results available to the community, in citable form, before we publish the edited article. We will replace this Accepted Manuscript with the edited and formatted Advance Article as soon as it is available.

You can find more information about Accepted Manuscripts in the <u>Information for Authors</u>.

Please note that technical editing may introduce minor changes to the text and/or graphics, which may alter content. The journal's standard <u>Terms & Conditions</u> and the <u>Ethical guidelines</u> still apply. In no event shall the Royal Society of Chemistry be held responsible for any errors or omissions in this Accepted Manuscript or any consequences arising from the use of any information it contains.



3 4 5 6 7 8 9 10 11 12 13 14 15ຊິ en de gesentricie. Publisbed on Ol de gentrand Romano de de nos 42023 94521 AM.
This article is licensed under a Creative Commons Attribution 30 On Soried Lice 45 46 47 48 49 50 51 52 53 54 55 56 57 58 59

60

View Article Online DOI: 10.1039/D2AN01350A

ARTICLE

Platform-agnostic electrochemical sensing app and companion potentiostat.

Received 00th January 20xx, Accepted 00th January 20xx

DOI: 10.1039/x0xx000000x

Viayalaxmi Manoharan, ^{a*} Rui Rodrigues, ^{a*} Sara Sadati, ^{a*} Marcus J. Swann, ^b Neville Freeman, ^b Bowen Du, ^a Ender Yildirim, ^c Ugur Tamer, ^d Theodoros N. Arvanitis, ^{a,e} Dmitry Isakov, ^a Ali Asadipour, ^{f†} and Jérôme Charmet, ^{a,g,h†}

Electrochemical sensing is ubiquitous in a number of fields ranging from biosensing, to environmental monitoring through to food safety and battery or corrosion characterisation. Whereas conventional potentiostats are ideal to develop assays in laboratory settings, they are in general, not well-suited for field work due to their size and power requirements. To address this need, a number of portable battery-operated potentiostats have been proposed over the years. However, most open source solutions do not take full advantage of integrated circuit (IC) potentiostats, a rapidly evolving field. This is partly due to the constraining requirements inherent to the development of dedicated interfaces, such as apps, to address and control a set of common electrochemical sensing parametres. Here we propose the PocketEC, a universal app that has all the functionalites to interface with potentiostat ICs through a user defined property file. The versatility of PocketEC, developed with an assay developer mindset, was demonstrated by interfacing it, via Bluetooth, to the ADuCM355 evaluation board, the open-source DStat potentiostat and the Voyager board, a custom-built, small footprint potentiostat based around the LMP91000 chip. The Voyager board is presented here for the first time. Data obtained using a standard redox probe, Ferrocene Carboxylic Acid (FCA) and a silver ion assay using anodic stripping multi-step amperometry were in good agreement with analogous measurements using a bench top potentiostat. Combined with its Voyager board companion, the PocketEC app can be used directly for a number of wearable or portable electrochemical sensing applications. Importantly, the versatility of the app makes it a candidate of choice for the development of future portable potentiostats. Finally, the app is available to download on the Google Play store and the source codes and design files for the PocketEC app and the Voyager board are shared via Creative Commons license (CC BY-NC 3.0) to promote the development of novel portable or wearable applications based on electrochemical sensing.

Introduction

Electrochemical sensing represents a growing field of research that has expanded through the development of novel materials and sensing modalities. With such developments, new applications have started to emerge including for remote or on-site sensing.

Applications include biosensing^{1–4}, environnemental monitoring^{5–8}, or battery characterisation^{9–13} to cite a few. Such applications are now constrained by the use of expensive and bulky desktop potentiostats, usually developed and tailored for laboratory settings and that are not well suited for wearable or portable applications.

To overcome these limitations, a range of small potentiostats were reported in the literature in recent years, alongside a few commercial options. Several custom-built platforms using discrete analogue components interfaced with dedicated microcontroller units (MCU) have been reported^{14–17} and, more recently, others took advantage of commercial analogue front end (AFE) or systems on chip (SoC) potentiostat integrated circuits (ICs). These can provide advanced functionality in a much more compact format, and greatly simplify development of new solutions. Projects based around the LMP91000 AFE (Texas Instruments), an IC used in a range of commercial portable potentiostats¹⁶, were reported in the literature^{18–21}. The Analog Devices ADuCM355 SoC with integrated microcontroller, which equips commercial product (see e.g. 22), has also been exploited recently to detect aptamers/ligand binding²³ or sweat rate and salt concentration therein²⁴. One issue with potentiostat IC is their specific communication protocols that put constraints on the development of dedicated interfaces.

Even though open source potentiostats, with wired connection, have been reported previously (e.g. to computers via serial

- Institute of Digital Healthcare, WMG, University of Warwick, Coventry, CV4 7AL, UK
- 5D Health Protection Group Ltd., Accelerator Building, 1 Daulby Street, Liverpool L7 8XZ. UK
- Middle East Technical University, Mechanical Engineering Department, 06800, Ankara, Turkey
- d. Department of Analytical Chemistry, Faculty of Pharmacy, Gazi University, Ankara, 06330, Turkey.
- e. School of Engineering, University of Birmingham, Edgbaston, Birmingham, B15 2TT, United Kingdom
- f. Computer Science Research Centre, Royal College of Art, London, SW7 2EU, United Kingdom.
- Warwick Medical School, University of Warwick, Coventry, CV4 7AL, UK
 School of Engineering-HE-Arc Ingénierie, HES-SQ University of Applied
- h. School of Engineering-HE-Arc Ingénierie, HES-SO University of Applied Sciences Western Switzerland, 2000 Neuchâtel, Switzerland.
- * These authors contributed equally to the work.
- † Corresponding authors.

Electronic Supplementary Information (ESI) available: [source code for the PocketEC app, source code for the Voyager board, source code for the ADuCM355 board, design files and bill of materials for the Voyager board, a sample priority file and app screenshots https://github.com/Pocket-EC]. See DOI: 10.1039/x0xx00000x

Figure 1. Schematic of the PocketEC app communicating, via Bluetooth, with MCU based potentiostats. We demonstrate communication with established platfoms such as the DStat as well as a custom-made Voyager board and the commercially available EvalADuCM355 board. An Arduino board was used to act as buffer between the DStat and the PocketEC app as the latter was designed for real-time communication and the former requires a buffer.

communication^{15,18,25–28} or smartphone via the audio jack²⁹) most applications are based on wireless communication protocols, usually with smartphones or tablets via Bluetooth, BLE^{14,30,31}, WiFi^{16,32,33} or NFC³⁴. Wireless communication, for control and/or data acquisition, enables small footprint, battery-operated, potentiostats to be used in enclosed spaces as well as for wearable applications¹⁴. Smartphones, whose use is now widespread including in resource limited settings³⁵, are a candidate of choice due to their ever increasing computing power, the possibility to share the results quickly, and back-end processing possibilities (e.g., in the cloud). Dedicated apps or web interfaces are typically used to communicate with the potentiostats. Apps provide fully integrated solutions, however their development requires a specific set of skills, and their use is typically limited to one dedicated potentiostat. Bearing in mind that most developments rely on established electrochemical sensing assays, each app proposes similar interfaces and parameters to setup and control the assays. Indeed, the main difference between most apps lies in the communication protocol with their dedicated potentiostats. Consequently, significant development effort is lost on the (re)programming of a set of common, cross-platform settings each time a new potentiostat is proposed. This process could be greatly simplified through the development of a versatile app comprising a set of pre-programmed electrochemical settings and programmable communication protocols.

1 2 3

4

5

6 7

8

9

10 11 12

13

14 15

Rownloaded on 8/42023 9:45:21 AM - Commons Attribution 3:0 Unported Lice

acese Article Published on (1)

45

46

47

48

49

50

51

52

53

54 55

56

57

58

59 60 Finally, most solutions proposed to date were developed from an electrochemical research point of view and whilst providing the fundamental measurement data, stop short of the conversion to the desired result required to make the measurement accessible to a wide audience. For example, most platforms report current or voltage depending on the assay, whereas a concentration would be most appropriate for biosensing assay development.

With the above considerations in mind, we propose an integrated solution comprising of 1) the PocketEC, a universal app, that can potentially be made compatible with any potentiostat chip without any reprogramming, 2) the Voyager board, a versatile miniature potentiostat, and 3) an intermediary data communication Arduino-based platform for third-party potentiostats with buffer-stored data.

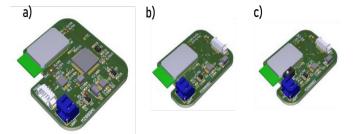


Figure 2. The Voyager board design variant; a) single-sided board, b) double-sided board, and c) double-sided board with mode sliding switch to select between two and three electrode configuration.

The user-friendly PocketEC app, the main focus of the paper, has the following attributes: i) It is based on a novel concept that makes it easier to use with a range of potentiostats; it uses a JSON property file to address firmware and hardware specific commands, making it usable with a range of potentiostats as demonstrated here using the custom-made Voyager board, and the commercially available ADuCM355 evaluation board, and the open-source DStat potentiostat. Each board harbours unique AFEs and MCUs; Voyager board (PIC24F MCU and LMP91000 AFE) and ADuCM355Eval board (ARM Cortex M3 MCU and ADuCM355 AFE), and DStat board (ATxmega256A3U MCU and discrete elements AFE) chosen to highlight the versatility of the PocketEC app. ii) It contains a calibration procedure that can be used pre- or post-measurement to convert the results into context-relevant units such as concentration and iii) it proposes a set of flexible parameters that allow the user to create and recall a wide range of user defined electrochemical techniques to condition electrochemical sensors and measure their responses. Finally, iv) the app is available on the Google Play Store and its source code is available via Creative Common License (CC BY-NC 3.0). The small footprint (< 14 cm²) Voyager board, based around the LMP9100 AFE i) is battery operated, ii) communicates with the app via Bluetooth and iii) its source code and design files are made available via Creative Common License (CC BY-NC 3.0). The Voyager board, presented here for the first time, provides a simple interface that will work with the PocketEC app without any reprogramming.

We demonstrate the versatility of the app, by measuring an amperometric Ferrocene Carboxylic Acid (FCA) assay on the DStat potentiostat, on the ADuCM355 evaluation board, and on the custom-made battery-powered Voyager board (Figure 1). We also compare the results from the voyager board with a commercial

3

4

5

6

7

8

9

10

11

The Gese Anticle Published and Languer 1913 Rownloaded and 84521 AML The afficies Beened and a Creative Commons Kitching 30 6 moored Lice

44

45

46

47

48

49

50

51

52

53

54

55

56

57

58

59 60 ARTICLE

benchtop laboratory potentiostat (Digi-IVY 2322, US) for the FCA assay as well as for a silver assay using anodic stripping. Our results demonstrate the versatility of the PocketEC app that can seamlessly communicate with the portable potentiostats. They also show good agreement between the tabletop potentiostats and the voyager board with calibration curves exhibiting very good linearity, and <1% difference in slope.

Methods

App architecture and programming.









is based on the ADuCM355, an on-chip system that controls and

measures electrochemical sensors and bioseosors.10ts9ntegrates5an

ARM Cortex M3 microcontroller, 16-bit 400kSPS ADC, programmable

gain amplifier, antialiasing filter and AFE. The Digital-to-Analog

Converters (DACs) which control the noninverting inputs of the

potentiostat amplifier and the transimpedance amplifier (TIA) output

voltage from 0.2V to 2.4V with at least 0.54 mV resolution. The TIA is

suitable for measuring current output from ±0.00005 μA to ±3000 μA

and the load and gain resistors of this TIA are programmable. The



Figure 3. The PocketEC app proposes a flexible interface to communicate with a range of potentiostats and enables the creation and recall of multi-techniques conditioning and measurement steps. Screenshots of the main features with the Methods, Charts, Calibration and Analysis sections.

The hybrid mobile app was developed using Ionic Framework 3, so that the same code for the mobile app can be used in multiple mobile platforms. The link to the source code is provided in the Supplementary Materials. The app, available on Google Play Store, was tested on several Android based smartphones and tablets from Samsung Galaxy S7 (Android 7) to Google Pixel4 (Android 12). It may also be compiled for iOS and Windows. In the case of iOS, the potentiostat must use Apple's MFi technology to connect to the phone.

Voyager board.

The Voyager board is based around the Integrated Analog Front End (AFE) potentiostat - LMP91000 by Texas Instruments³⁶. It has an internal programmable control logic module with three control registers (CNs); TIA control register (TIACN), reference control register (REFCN), and mode control register (MODECN). An integrated temperature sensor is available to reduce noise caused by ambient temperature variations. A PIC24F microcontroller with 12bit ADC modules was chosen to drive the LMP91000 via an I2C connection. This MCU is used across a broad range of industrial applications which enables enhanced accuracy in sampling, and reliable wireless communication with the app. The code was programmed in C using the MikroElektronika's integrated development environment (IDE)37. Three prototype boards were designed and fabricated in-house (Altium Designer) as shown in Figure 2. The final design, reported herein is a double-sided board with mode sliding switch to select between two and three electrode configuration. The PCB layout design and firmware are provided in the Supplementary Materials.

Evaluation board.

We used the evaluation board EVAL-ADUCM35538 by National Instruments to demonstrate the universality of the PocketEC app. It measurement possible in ADuCM355 based solutions. The large output voltage range, ability to implement most electrochemical sensing modalities, highly integrated design and highly controllable circuitry makes this platform a candidate for wide implementation in research settings and in platforms requiring multi-sensing capabilities.

Functions required for control of the potentiostat and communication with the PocketEC app were implemented using the M355_ECSns_SingleWE example provided by AD³⁹ as reference. This implementation allows for the setting of TIA gain resistor, load resistor, voltage bias and voltage zero values relevant for channel 0. The code is provided in Supplementary Materials.

DStat board.

The DStat board is built around the ATxmega256A3U microcontroller (Microchip Technology, San Jose CA, USA)⁴⁰. It has a potentiostat circuit that uses a transimpedance amplifier (TIA) with programmable gain ranging from 100 Ω to 500 $M\Omega$ for current measurements. The circuit is designed with an additional unity gain amplifier, to limit the current flow through the reference electrode (RE). An external 16-bit DAC unit is integrated with a step size of 46 μV for the 0–3 V range. DStat board utilises a 24-bit ADC, which is integrated with a digital antialiasing filter for reduced noise measurements. Due to the high resolution of the ADC, the instrumental limit of detection for current measurements is approximately 600 fA. The maximum current output with the lowest gain resistor (100 Ω) is 15 mA, offering a large output range.

The potentiostat circuit can perform various types of electrochemical measurements, including chronoamperometry, cyclic voltammetry, differential pulse voltammetry, square wave voltammetry, and potentiometry. The board, initially developed for wired

48

49

50

51

52

53

54

55

56

57

58

59 60

1

3

4

5

6

7

Journal Name ARTICLE

communication, was reprogrammed following the open access instructions⁴¹, and by using the Olimex AVR ISP Mk2 external programmer to enable wireless communication. The new firmware code is provided in Supplementary Materials.

Arduino board.

We used an Arduino Mega 2560 microcontroller board as a buffer platform for the non-real time measurements of DStat potentiostat. Indeed, our app was designed to account for more demanding real-time measurements, however, consequently it cannot handle buffered data. The choice of well-established and widely available Arduino boards is to ensure an easy integration with other platforms. The Arduino integrated development environment (IDE) 1.8 was used to program the Arduino board. The Arduino sketch is also provided in Supplementary Materials.

electrode was transferred back to PBS and connected to the test potentiostat. The working electrode was poised at \$0000 MV for \$20 seconds, 450 mV for 20 seconds and 50 mV for 20 seconds with respect to the reference electrode. The electrode was then held at 50mV for 180 seconds. The solution was stirred for a minimum of 60 seconds at the beginning of the final 50 mV step. The process was then repeated ensuring that measurements were only taken after the solution had been allowed to stand for more than 60 seconds. The measurement in PBS was repeated five times to allow the baseline value to stabilise and then FCA stock solution was added to produce a 0.001 mM solution and the procedure repeated. Duplicate measurements were then taken at 0.003, 0.01, 0.03, 0.1 and 0.3 mM respectively to produce a calibration curve. The procedure was repeated with a commercial laboratory potentiostat for comparison.

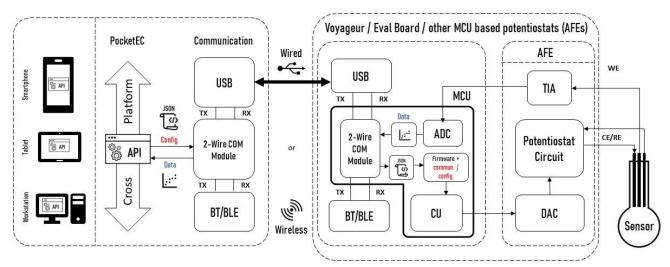


Figure 4. Typical architecture of a complete system for wired and/or wireless solutions. The parts in red indicate the platform dependent configuration and communication classes that need to be implemented.

Electrochemical sensing.

Sensor Electrodes. Electrochemical assays used commercially available gold sensor electrodes with an integral silver reference electrode and gold counter electrode (Dropsens, Metrohm, UK). Individual sensors were first prepared to ensure reproducible behaviour for experiments across different potentiostats. They were prepared by first removing traces of silver from the working electrode which was occasionally observed, presumably from the fabrication process. This was done by cycling the working electrode between -0.1 and +0.5 V at 50 mV/s, five times, in 50 mM NaNO $_{\mbox{\tiny 3}}$ in high purity (>18.2 M Ω) water. The potential of the silver reference electrode was also observed to vary between different sensors when compared to a standard Ag/AgCl reference electrode (BAS, Metrohm, UK) or the measured FCA redox potential. This was minimised after chloridisation, which was achieved by holding the reference electrode at 0.2 V vs. an external Ag/AgCl reference electrode (BAS, Metrohm, UK) for 30 s in 0.1M NaCl(aq) solution.

Amperometry. Ferrocene Carboxylic Acid (FCA). A stock solution of 1 mM FCA (Sigma-Aldrich, UK) in Phosphate Buffered Saline (PBS, pH7.4) (Sigma-Aldrich, UK) was made up using deionised water. A prepared gold electrode (Dropsens, Metrohm, UK) was immersed in PBS solution, pH 7.4, and connected to a laboratory potentiostat (Digi-Ivy). The sensor performance was first checked by cyclic voltammetry in PBS and 1 mM FCA solution. Following this the

Anodic Stripping Multi-step Amperometry. A stock solution of silver nitrate (10 mM) in sodium nitrate (50 mM) and nitric acid (10 mM) was made up in deionised water. The solution was made up fresh and stored in the dark prior to use. A prepared gold electrode (Dropsens, Metrohm, UK) was connected to the potentiostat (Digi-Ivy or Voyager board respectively) and the electrode immersed in a solution of 50 mM sodium nitrate and nitric acid (10 mM). The following working electrode potential sequence was used: 0.5 seconds at 0 V, 50 seconds at -200 mV, 100 seconds at 0.200 mV. When integrating the charge, the 100 seconds (stripping) step at 0.200 mV was split into 5 seconds and 95 seconds, the 5 second measurement being used for the analysis. After repeating the blank measurement, additions of stock silver solution were added to produce silver solutions of 0.003, 0.01, 0.03, 0.1, 0.3, 1, and 3 mM respectively with duplicate measurements for each concentration. The solutions were stirred between each measurement and after each addition and allowed to settle for at least a minute between measurements. The data were used to construct a calibration curve

Results and discussion

PocketEC App and communication protocol

PocketEC App: The PocketEC app was designed to provide a simple user experience. It comprises three sections for 1) controlling the device (Settings), 2) real-time visualisation of measurements (Charts) and 3) processing of stored data (Analysis). Figure 3 shows selected

3

4

5

6

7

8

9

10

11

12

13

14

en Access Article, Published and August 2043 Bawalonde Con & 42023 945-21 AM 1 This article is the need inder a Cearitye Commons Kirrbuiton 5.0 Engerted Liberice.

44

45

46 47

48

49

50

51

52

53

54

55 56

57

58

59

60

ARTICLE

screenshot of each module. In the Settings module, the user 1) configures the app to communicate with the potentiostat by setting firmware specific communication parameters and 2) defines commands to be sent via Bluetooth Serial communication to preconfigure the device with the experimental parameters. Upon reception, the device starts the measurements and sends the data points back to the app, which stores them with a timestamp. The frequency at which the data is sent back is defined by the user and can therefore allow for near real-time visualisation. This feature facilitates new experiment designs and troubleshooting. Temperature is recorded at the end of each measurement cycle, allowing for temperature-dependent drifts to be accounted for.

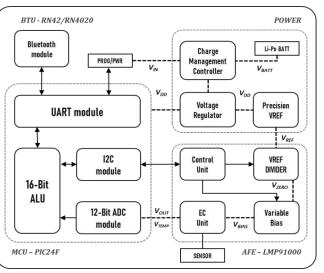


Figure 5. Voyager board block diagram.

Importantly, the app provides all the functionality required to communicate with a range of MCU-based potentiostats. This unique feature is enabled by the provision of a universal editable property file that defines the communication rules between the app and potentiostat. This user-editable file is all that is needed on the app side to enable communication with the potentiostats. A sample property file, specified in JavaScript Object Notation (JSON) - a standard text-based format for representing structured data, is shown in Supplementary Materials. On the MCU code, it suffices to add a configuration and communication class. Figure 4 shows the typical architecture of a complete system for wired and/or wireless solutions. The communication is independent from the AFE or MCUs used since all wired or wireless solutions use the 2-wire serial communication module (TX/RX). The only parts that need to be edited to allow full communication are shown in red.

Communication protocol: The app communicates with the potentiostat via Bluetooth. To start using a new potentiostat with the app, the user needs to perform a one-time process of linking the potentiostat to the app. This is done in the app's SETTINGS (Fig 3 a) by scanning for devices. Once a link is established the app is configured to communicate with the potentiostat in two stages. The first stage sets up fundamental rules of two-way communication between the app and the potentiostat. This is as specified by the properties in the JSON file described earlier. The second stage

configures the measurement cycle required for view maning man electrochemical assay, which can be made on of lone for multiple electrochemical techniques. Each technique specifies the voltage to be applied to the potentiostat, duration of applied voltage and the frequency at which the generated output voltage is sampled. All experimental parameters required for an assay can be saved as a Method and can be referenced again later. Multiple methods can be created and stored in the app and old methods can be edited and reused (see figure 3).

Once a method is created, an experiment can be started from the app. The app communicates with the potentiostat and sends commands as set in the Method by the user. At user specified intervals, the app requests data from the potentiostat which are stored on the phone with a timestamp. The collected data are processed and are available to view in near real-time. Compared with other approaches that rely on sequential communication, where the full protocol is typically sent to the potentiostat followed by the resulting timeseries being returned to the app at the end of the experimental run, we have opted for an approach allowing for near real-time monitoring. While this approach is particularly well suited for assay developments as it enables seamless troubleshooting and fine-tuning, it comes with its own challenges. As an example, the AduCM355 includes three sequencers that can be used to program instruction sets. Although this strategy provides good control over the experimental timing it also results in an overhead during development. Indeed, an intermediate representation of the protocols must be created, sent to the potentiostat device, and interpreted before its execution.

To avoid this, the PocketEC app is responsible for timing experimental steps, sending the minimal viable instruction set for execution of a particular experimental step in the potentiostat. In a reasonable experimental setup where the Bluetooth module of the host device is not under significant traffic, the delays introduced between instructions produced by the app and received by the potentiostat's internal logic should be consistent and will not introduce any significant error in the data collected.

Another unique feature of the app is the *Calibration module* that enables the user to view the data in application-specific units such as concentration. This feature, also available in real-time, is achieved via manual entry of sensitivity and offset parameters, or via on-board calibration measurement. This is particularly useful for non-experts who may struggle to make the link between the data and the expected measurement otherwise. Data analysis can also be carried out externally. Options to export the saved data in CSV (comma separated values) format by email, Bluetooth and other sharing methods are available. The detailed communication protocol and measurements steps are provided in Supplementary Materials.

Voyager board

Key design requirements were identified to prototype a preliminary solution (hardware and software), test its usability in a lab setting, and refine it in a circular design as detailed below. We first designed a one-sided board with a Bluetooth module (RN42APL by Microchip Technology⁴²) shown in Figure 2a as a proof-of-concept prototype. Following successful evaluation (data not shown), we designed and fabricated a smaller footprint option consisting of a double-sided board (Fig. 2b). Switches and configurable components added to the

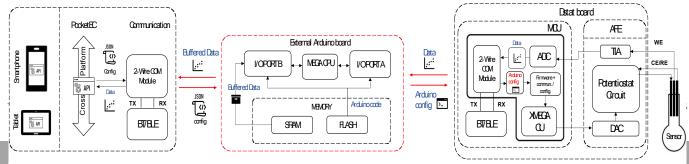


Figure 6. Block diagram for DStat measurements setup. The red areas indicate the additions made to the previous architecture.

nalyst Accepted Manusc

57

58 59 60

ARTICLE Journal Name

third version (Fig. 2c) enable the board to be used in different electrochemical or biomedical scenarios. The general block diagram of the Voyager boards is shown in Figure 5. The chip was programmed in-house to provide remote configuration and various data transfer modes (e.g., on-demand, burst, and pre-defined intervals) over wireless communication. The source code is available in Supplementary Materials. Lithium Polymer batteries (Li-Po) were purchased with different capacities to test and compare them against the simulated results outside a lab setting (experimented). The Voyager v3.0 is a small footprint board suitable for wearable applications. The source code, design files and bill of materials are given in Supplementary Materials.

Evaluation board

Implementation of a new sensing platform is likely to make use of stable evaluation platforms provided by the IC manufacturer at early stages. However, these evaluation platforms are typically designed for wired communication with a computer-based interface, being a limited proxy for the development of solutions that require and are limited by a wireless communication protocol, and that communicate with a mobile app. To validate our approach, we have selected the ADuCM355 evaluation board.

To communicate with the PocketEC app, a HC-06 Bluetooth module was interfaced to the evaluation board by removing the jumpers (JP45 and JP46) connecting the AduCM355 and UART-to-USB ICs and connecting the Rx and Tx signals to the HC-06 board. The BT module was powered via the JTAG connector header. The module's baud rate was changed to match the AduCM355's using AT commands provided by the manufacturer. By using a module capable of transparent UART communication, minimal setup was necessary. The approach would be similar upon future implementation of a BLE solution. No significant delays in communication were observed when compared with the Voyager board.

DStat potentiostat

To further validate the versatility of the PocketEC app, interface it with DStat, a well-established MCU-based open-source potentiostat²⁶. Initially designed to interface with a custom computer-based platform using wired communication (USB), DStat required modifications to enable seamless communication with a mobile app via Bluetooth. This was achieved by replacing USB communications device class (CDC) with USARTCO port in XMEGA MCU to enable serial communication via Rx/Tx signals.

The PocketEC app was designed to enable near real-time communication, which is fundamentally different from the DStat communication protocol designed to receive all the experiment specifications before execution. To address this disparity, an intermediate Arduino-based platform was integrated into the system. The platform was programmed to receive the complete experimental parameters protocol sent by the PocketEC app and subsequently relay it to the DStat. Additionally, the platform acts as a buffer to store the measurements acquired by DStat and transmitting them individually to the PocketEC app upon request. Arduino Mega board⁴³ with 4 UART hardware ports was utilised for the two serial communications. Specifically, Tx1/Rx1 pins were connected to UART port C on DStat board, and Tx2/Rx2 were dedicated to the HC-06 Bluetooth module. Like with the ADuCM355 evaluation board and the Voyager board, no significant delay was observed upon connection. Figure 6 shows the established architecture created for DStat measurements.

The Arduino board was also programmed for data processing including the conversion of ADC and DAC units to desired/amperes and volts units. These fundamental conversions were originally applied on the computer-based interface developed for DStat. However, to minimise the changes on the app settings, they were applied on the Arduino platform. The Arduino board was further programmed to address the difference in time intervals for measurements. While this parameter is a user-defined value that determines the frequency at which data is sent back to the app, this value is set by the DStat ADC sampling rate. The Arduino board was programmed to send the average of several subsequent data points based on the user-defined value, thus bringing the time intervals into close agreement.

This novel integration between the PocketEC app and DStat potentiostat showcases their compatibility and establishes a seamless connection for efficient potentiometry analysis. This near real-time measurement setup, using and Arduino platform, was created to overcome the substantial disparities in communication protocols. By implementing this approach, similar adaptations can be effortlessly applied to other potentiostats that rely on receiving complete experiment parameters prior to execution. This implementation ensures compatibility without necessitating reprogramming on either the app or a potentiostat, making it a flexible and scalable solution for diverse potentiometry applications.

Overview of the communication with different platforms

Above, we have seen how the PocketEC app can be interfaced with different potentiostats. This was done without any reprogramming of the app, thanks among others to its JSON configuration file. This file is used to set up fundamental rules of two-way communication between the app and the potentiostat; format of transmission of commands from app to the potentiostat, expected format and length of data received from potentiostat and listing of all possible values that can be used to program the control registers of the potentiostat. The properties in the JSON file are described in Table 1. The app contains a list of JSON properties with default values. These properties can be edited by the user via SETTINGS and set with potentiostat dependent values. These properties need to be set just once for every potentiostat or whenever there are firmware updates in the potentiostat. Multiple JSON configurations can be created and stored in the app. Sample JSON files are provided for each of the 3 potentiostats used here. After this initial communication configuration step, the configuration of the potentiostats, as described above, can take place.

As mentioned above, although the PocketEC app does not require additional changes, some programming adjustments are necessary on the potentiostats' side to accommodate for microcontrollerspecific settings. However, using manufacturers recommended codes (see e.g., reference³⁹ for the AduCM355), it becomes feasible to address the required registers for real-time measurements. To facilitate buffered communication, we have proposed to use an Arduino board to handle the register addressing buffering. Table 2 shows the main parameters for managing these settings with corresponding examples for three potentiostats that were connected to the PocketEC app in this study.

Electrochemical measurements

For the app and board development, the decision was taken to read the raw data from the board and process it in the app. This is to minimise the level of computation and data analysis required on the board, which will help minimise the complexity and cost of

ARTICLE

development. One consequence of this however is that where the data acquired is time dependent, this needs to be accounted for. For

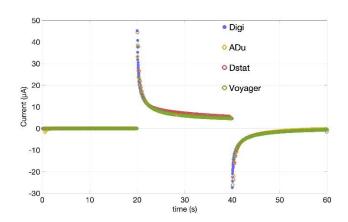
View Article Online DOI: 10.1039/D2AN01350A

 Table 1. JSON configuration parametres.

Electrochemical relevance	Variable/ property name	Comments	Example Values
Gain (used to define the current range)	TIACN control register	Transimpedance amplifier resistor based on the values dependant on the AFE circuit	Voyager board, 2.75KΩ to 350KΩ, 35KΩ used for CA measurements. EvalADuCM355, 0 to 512KΩ range, 32KΩ used for CA measurements. DStat, 100 to 100M range, 30KΩ used for CA measurements.
Load Resistance	TIACN control register	Programmable resistive load that also affects the gain	• Voyager board, 10Ω to 100Ω range, 10Ω used for CA measurements. • EvalADuCM355, 0 to 3.6 KΩ range, 10Ω used for CA measurements. • DStat, not defined
Applied voltage	REFCN control register	Experiment-dependant bias voltage applied to the electrochemical cell at each step	Voyager board, ±0.6V at 0.05V intervals with programmable percentage of the source reference (20%, 50%, 67%) EvalADuCM355, ±0.6V at 0.05V intervals DStat, ±1.5V range
Voltage duration	Duration (s)	Duration of the applied voltage at each step	Experiment-dependant. Default value 3s in the Methods section
Operational mode	MODECN control register	Defined to set the board in a potentiostat 3-lead mode	Voyager board, this value is set to 3 by default EvalADuCM355, 3 DStat, not defined
Sampling Rate	Data frequency (ms)	Defines how fast the potentiost collects measurement values	 Voyager board, this value is set to 200ms by default EvalADuCM355, 200ms DStat, ~200ms adjusted by averaging
Temperature sensor	readTemperature property	Integrated temperature sensor measurements	Voyager board, temp value sent in bytes at the end of each step EvalADuCM355, temp values sent in String DStat, not integrated

Table 2. Communication protocols

Property Name	Description	Example Values
responseDelimiter	Expected string at the end of all communications from	"\r\n"
	Potentiostat to app when format of communication is	
	String	
Test	The property value pairs included in this property specify	"Tx": ""
	communication rules between app and Potentiostat in Test	"TxAsString": true
	mode when the Potentiostat is linked to the app the first	"RxAsString": true
	time.	"RxLength": "3"
readData	The property value pairs included in this property specify	"Tx": "3"
	communication rules between app and Potentiostat for	ring": true
	reading data.	"RxAsString": false
		"RxLength": "3"
readTemperature	The property value pairs included in this property specify	"Tx": "2"
	commands and communication rules and between app and	"TxAsString": true
	Potentiostat for reading temperature.	"RxAsString": true
		"RxLength": null
setConfigMode	Specifies the command required for setting the	"Tx": "0",
	Potentiostat into configuration mode where it expects the	"TxAsString": true,
	next command to contain commands for setting its	"RxAsString": false,
	registers. In this example '0' sets the potentiostat in config	"Rx": "Send Three Bytes",
	mode. TxAsString should be set to true if app sends the	"RxLength": "18",
	command '0' as a string to the potentiostat. RxAsString	
	should be set to false if expected reply should be read as	
	bytes. Rx specifies expected reply from the Potentiostat	
	and RxLength the length of the expected bytes in the reply	
setRegisters	This property defines the communication format and	"Tx": null,
	expected reply when the app sets the registers of the	"TxAsString": false, "RxAsString": false,
	potentiostat	"Rx": "TIACN OK\r\nREFCN OK\r\nMODECN OK",
	· ·	"RxLength": "31"
REFCN	Lists all values that can be used to set the Reference	{"description":"20%",
	control register	"SETTING": [
		{"description":"0.6V 20%","command":"157"},
		}



Journal Name

1 2 3

4

5

6

7

8

9 10 11

12

13

14

15ຊິ

pen Access Article, Published and Laugust 2013 Rown order on 842013 945-21 AM - Ansarticle, Published and Accessive Commons Kirrbuiton 30 On Borted Lice

44

45

46

47

48

49

50 51

56

57

58

59 60

Figure 7. Amperometric measurement for 1mM FCA in PBS. Voltage applied 0.05 V 0-20 s, 0.45 V 20-40 s and 0.05 V 40-60 s. Measurements with commercial laboratory potentiostat (Digi), Voyager board, DStat board, and ADuCM355 evaluation boards (ADu). Because the acquisition rate is lower for the development boards, the initial datum at each transition is offset to the mid time-point of the acquisition.

the Voyager board once a potential is applied, the ADC is read continuously, dictated by the microcontroller duty cycle, and the

result added to a running tally. When the value is read by the app, it transfers the average value and the number of times the ADC has been read. So, the value read represents an average current (bits)

value over the whole-time interval since the last reading, rather than an instantaneous value which could vary according to differences in the exact timing. This is especially important where, for example, the current passed was decaying significantly in the time-period following a potential step, as is often the case.

During the analysis, where the charge passed is calculated from the data acquired during a defined amperometric measurement step, the actual accumulated time for the step can vary by up to the length of the repeat time. This is accounted for by scaling the time interval and charge of the last point to ensure that the calculated charge is measured over the same total time period.

The applicability of the app across multiple development boards was demonstrated using an amperometric measurement of the redox mediator FCA in PBS. Data from the Voyager, and ADu, and DStat boards were compared with data from a commercial laboratory

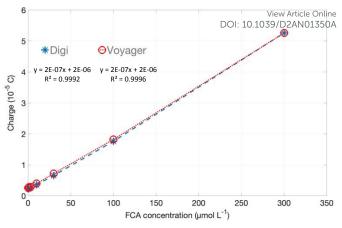


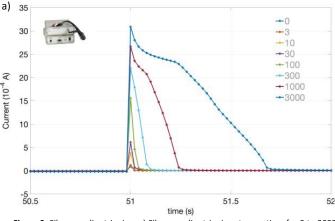
Figure 8. Calibration assay for FCA. Charge vs. concentration, 0 to 300 μM FCA in PBS using amperometric measurement shown in Figure 6. The error bars show the range of the duplicate measurements. They are within the size of the markers, so are plotted but not visible.

potentiostat, shown below. The current sensitivities for the Voyager board were calibrated using an external dummy cell with selectable resistors.

Amperometry: Figure 7 shows the oxidation current passed during an amperometric I-t measurement for the Au electrode in a 1 mM FCA stock solution, at 0.45 V for 20 s, followed by a step to 0.05 V for 20 s. The data from the Voyager, ADU, and DStat boards (200 ms interval) are superimposed on the data from the commercial potentiostat (interval 20 ms) and show very good correlation.

To compare differences between the measurements obtained with the app/development boards and a laboratory potentiostat, more detailed comparisons were made using the Voyager board. The FCA stock solution and the same measurement procedure was used to create a calibration curve for FCA in PBS, shown in figure 8. Here the charge passed during the 20 s oxidative step was calculated for each measurement. The two data sets are barely distinguishable, with <1% difference in the slope, demonstrating the performance of the Voyager board.

Anodic Stripping: The Voyager and Digi-Ivy potentiostats were also compared for an Ag anodic stripping multi-step amperometry measurement. This is a more challenging situation, as Ag is collected on the working electrode during an extended reduction phase,



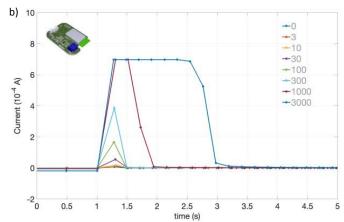


Figure 9. Silver anodic stripping. a) Silver anodic stripping step vs. time for 0 to 3000 µM AgNO₃ using commercial laboratory potentiostat, acquisition time 20 ms. b) Silver anodic stripping step vs. time for 0 to 3000 μM AgNO₃ using Voyager board. Acquisition time 200 ms, 2.7 kOhm range, 100 Ohm load resistor.

46

47

48

49

50

51

52

53

54

55

56

57 58

59

60

Journal Name ARTICLE

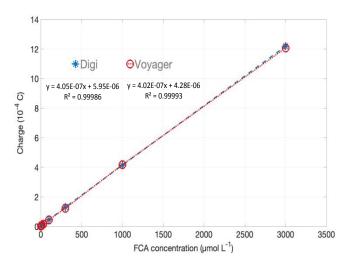


Figure 10. Silver anodic stripping calibration plots for commercial tabletop potentiostat (Digi) and Voyager board. Integrated charge vs. Ag* concentration. The error bars show the range of the duplicate measurements. They are within the size of the markers, so are plotted but not visible.

traditionally accompanied by rapid stirring, and is measured by reoxidising the deposited Ag, which occurs as a high current pulse over a short period of time. Using the relatively large DropSens Au sensor electrodes, this current saturated the range of the Voyager board.

The overlaid anodic stripping currents are shown in figure 9. In figure 9a, using the laboratory potentiostat we can see that up to 300 μ M Ag $^{+}$, the oxidative charge is passed within 100 ms. After this the time taken extends as more than a monolayer of Ag 0 is deposited and this slows the oxidation process down.

Figure 9b shows the equivalent data obtained with the Voyager board. As the acquisition interval is 200 ms, this is slower than the oxidation current spike, however the average value is captured by the faster on-board measurement and integration. As the current has saturated, the current is passed over a longer period of time for the higher Ag $^+$ concentration values. This takes 2 s at 3 mM Ag $^+$, compared to $^{\sim}0.7$ s with the laboratory potentiostat.

The calibration curves for the two potentiostats are overlaid in figure 10, and both show very good linearity with <1% difference in slope between the two devices. Overall, the comparison between measurements using the Digi-Ivy potentiostat and Voyager boards show very good agreement even where the timescale of the app acquisition or the current range of the Voyager board are limited. It should be noted that this has relied on pretreatment of the Au sensors to make their performance sufficiently reproducible.

Conclusions

In this manuscript, we have presented the PocketEC, a platformagnostic app tailored for wearable or portable electrochemical sensing applications. The app, optimised for assay development, can communicate seamlessly with several IC based potentiostat platforms via a user-defined property file to address firmware and hardware specific commands. The advantage of such an approach is that the app can be used with several potentiostat ICs, including future generation of ICs with minimum programming investment.

The versatility of the app was demonstrated by interfacing it with two significantly different MCU based potentiostats, namely the commercially available ADuCM355 evaluation board, the open-source platform DStat, and the Voyager board to presented here for the first time. The boards were evaluated against a tabletop potentiostat by measuring an amperometric Ferrocene Carboxylic Acid (FCA) assay and a silver assay using anodic stripping. The results have shown excellent agreement, with calibration curves exhibiting good linearity and less than 1% difference in slope.

The PocketEC is available to download on the Google Play Store and the source codes for the app and the boards (Voyager, ADuCM355EVAL, and Arduino) are provided alongside the design files for the Voyager board. It is also noted that the PocketEC app can be compiled for iOS devices using Apples' MFi technology or for Windows Mobile. We anticipate that the results presented herein will promote the development of portable and wearable electrochemical sensing applications in fields including in-situ battery monitoring, wearable health monitoring devices or remote sensing applications to name a few.

Author Contributions

Conceptualisation: NF, MS, JC. Investigation, methodology: VM, RR, SS, AA, BD, UT. Validation: MS, NF, EY. Software: VJ, RR, AA. Supervision, TA, JC. Funding acquisition TA, AA, UT, EY, NF, DI, JC. Writing – original draft: RR, VM, SS, AA, MS, JC. Writing – review and editing all.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

The research presented in this manuscript was supported by the Newton Fund—Institutional Links grant (ID 352360246), a MICRA Commercialisation Development Grant Award, Innovate UK (Project Ref. 104512) and the High Value Manufacturing Catapult at the University of Warwick. Professor Theodoros N Arvanitis is partially supported by Health Data Research UK, which is funded by the UK Medical Research Council, Engineering and Physical Sciences Research Council, Economic and Social Research Council, Department of Health and Social Care (England), Chief Scientist Office of the Scottish Government Health and Social Care Directorates, Health and Social Care Research and Development Division (Welsh Government), Public Health Agency (Northern Ireland), British Heart Foundation and Wellcome Trust (HDR UK – Medical Research Council – Award Reference HDR-3001.)

We would like to thank Judith Klein Seetharaman and Narinder Sanghera for initiating the collaborations and fruitful discussions. We would like to thank Dr Andrew Ward (University of Strathclyde) for lending his DStat platform.

Journal Name ARTICLE

Notes and references

1

3

4

5

6

7

8

9

10

11

12

13

14

15

Bust 2013. Provided on 8/8023 9:45:21 AM. Commons Attribution 3:0 Unported Lice

(Gesse Article Publishedonの) Musers Article Publishedonの Muserticle Is licensed under

44

45

46

47

48

49

50

51

52

53

54

55

56

57

58

59 60

- (1) Russell, C.; Ward, A. C.; Vezza, V.; Hoskisson, P.; Alcorn, D.; Steenson, D. P.; Corrigan, D. K. Development of a Needle Shaped Microelectrode for Electrochemical Detection of the Sepsis Biomarker Interleukin-6 (IL-6) in Real Time. *Biosensors* and *Bioelectronics* 2019, 126, 806–814. https://doi.org/10.1016/j.bios.2018.11.053.
- (2) Dai, Y.; Liu, C. C. Recent Advances on Electrochemical Biosensing Strategies toward Universal Point-of-Care Systems. Angewandte Chemie 2019, 131 (36), 12483–12496. https://doi.org/10.1002/ange.201901879.
- (3) Torul, H.; Yarali, E.; Eksin, E.; Ganguly, A.; Benson, J.; Tamer, U.; Papakonstantinou, P.; Erdem, A. Paper-Based Electrochemical Biosensors for Voltammetric Detection of MiRNA Biomarkers Using Reduced Graphene Oxide or MoS2 Nanosheets Decorated with Gold Nanoparticle Electrodes. *Biosensors* 2021, 11 (7), 236. https://doi.org/10.3390/bios11070236.
- (4) Cesewski, E.; Johnson, B. N. Electrochemical Biosensors for Pathogen Detection. *Biosensors and Bioelectronics* 2020, 159, 112214. https://doi.org/10.1016/j.bios.2020.112214.
- (5) Hashem, A.; Hossain, M. A. M.; Marlinda, A. R.; Mamun, M. A.; Simarani, K.; Johan, M. R. Nanomaterials Based Electrochemical Nucleic Acid Biosensors for Environmental Monitoring: A Review. Applied Surface Science Advances 2021, 4, 100064. https://doi.org/10.1016/j.apsadv.2021.100064.
- (6) Zhou, Z.; Mukherjee, S.; Hou, S.; Li, W.; Elsner, M.; Fischer, R. A. Porphyrinic MOF Film for Multifaceted Electrochemical Sensing. *Angewandte Chemie International Edition* 2021, 60 (37), 20551–20557. https://doi.org/10.1002/anie.202107860.
- (7) Wu, F.; Zhao, J.; Han, D.; Zhao, S.; Zhu, R.; Cui, G. A Three-Electrode Integrated Electrochemical Platform Based on Nanoporous Gold for the Simultaneous Determination of Hydroquinone and Catechol with High Selectivity. *Analyst* 2021, 146 (1), 232–243. https://doi.org/10.1039/D0AN01746A.
- (8) Liu, Z.; Xia, X.; Zhou, G.; Ge, L.; Li, F. Acetylcholinesterase-Catalyzed Silver Deposition for Ultrasensitive Electrochemical Biosensing of Organophosphorus Pesticides. *Analyst* **2020**, 145 (6), 2339–2344. https://doi.org/10.1039/C9AN02546D.
- (9) Sun, G.; Yu, F.-D.; Zhao, C.; Yu, R.; Farnum, S.; Shao, G.; Sun, X.; Wang, Z.-B. Decoupling the Voltage Hysteresis of Li-Rich Cathodes: Electrochemical Monitoring, Modulation Anionic Redox Chemistry and Theoretical Verifying. Advanced Functional Materials 2021, 31 (1), 2002643. https://doi.org/10.1002/adfm.202002643.
- (10) Yang, H.; Chen, S.; Gong, L.; Zaman, S.; Qi, K.; Guo, X.; Qiu, Y.; Xia, B. Y. Online Electrochemical Behavior Analysis on the Negative Plate of Lead-Acid Batteries during the High-Rate Partial-State-of-Charge Cycle. *Electrochimica Acta* 2020, 354, 136776. https://doi.org/10.1016/j.electacta.2020.136776.
- (11) De Angelis, A.; Crescentini, M.; Ramilli, R.; De Angelis, G.; Tartagni, M.; Moschitta, A.; Traverso, P. A.; Carbone, P. A Compact System for On-Line Electrochemical Impedance Spectroscopy on Lithium-Ion Batteries. In 2020 IEEE International Instrumentation and Measurement Technology Conference (I2MTC); 2020; pp 1–6. https://doi.org/10.1109/I2MTC43012.2020.9128567.

- (12) Li, W.; Lutz, D. M.; Wang, L.; Takeuchi, K. J.; Marschiloke Andrée Takeuchi, E. S. Peering into Batteries: Electrochemical Nosigba Through In Situ and Operando Methods over Multiple Length Scales. *Joule* **2021**, *5* (1), 77–88. https://doi.org/10.1016/j.joule.2020.11.003.
- (13) Fleming, J.; Amietszajew, T.; Charmet, J.; Roberts, A. J.; Greenwood, D.; Bhagat, R. The Design and Impact of In-Situ and Operando Thermal Sensing for Smart Energy Storage. *Journal of Energy Storage* **2019**, *22*, 36–43. https://doi.org/10.1016/j.est.2019.01.026.
- (14) Ainla, A.; Mousavi, M. P. S.; Tsaloglou, M.-N.; Redston, J.; Bell, J. G.; Fernández-Abedul, M. T.; Whitesides, G. M. Open-Source Potentiostat for Wireless Electrochemical Detection with Smartphones. *Anal. Chem.* **2018**, *90* (10), 6240–6246. https://doi.org/10.1021/acs.analchem.8b00850.
- (15) Meloni, G. N. Building a Microcontroller Based Potentiostat: A Inexpensive and Versatile Platform for Teaching Electrochemistry and Instrumentation. J. Chem. Educ. 2016, 93 (7), 1320–1322. https://doi.org/10.1021/acs.jchemed.5b00961.
- (16) Bianchi, V.; Boni, A.; Fortunati, S.; Giannetto, M.; Careri, M.; De Munari, I. A Wi-Fi Cloud-Based Portable Potentiostat for Electrochemical Biosensors. *IEEE Transactions on Instrumentation and Measurement* 2020, 69 (6), 3232–3240. https://doi.org/10.1109/TIM.2019.2928533.
- (17) Gao, W.; Emaminejad, S.; Nyein, H. Y. Y.; Challa, S.; Chen, K.; Peck, A.; Fahad, H. M.; Ota, H.; Shiraki, H.; Kiriya, D.; Lien, D.-H.; Brooks, G. A.; Davis, R. W.; Javey, A. Fully Integrated Wearable Sensor Arrays for Multiplexed in Situ Perspiration Analysis. *Nature* 2016, 529 (7587), 509–514. https://doi.org/10.1038/nature16521.
- (18) Hoilett, O. S.; Walker, J. F.; Balash, B. M.; Jaras, N. J.; Boppana, S.; Linnes, J. C. KickStat: A Coin-Sized Potentiostat for High-Resolution Electrochemical Analysis. *Sensors* **2020**, *20* (8), 2407. https://doi.org/10.3390/s20082407.
- (19) Kaushik, A.; Yndart, A.; Jayant, R. D.; Sagar, V.; Atluri, V.; Bhansali, S.; Nair, M. Electrochemical Sensing Method for Point-of-Care Cortisol Detection in Human Immunodeficiency Virus-Infected Patients. *Int J Nanomedicine* 2015, 10, 677–685. https://doi.org/10.2147/IJN.S75514.
- (20) Azimi, S.; Farahani, A.; Docoslis, A.; Vahdatifar, S. Developing an Integrated Microfluidic and Miniaturized Electrochemical Biosensor for Point of Care Determination of Glucose in Human Plasma Samples. *Anal Bioanal Chem* 2021, 413 (5), 1441–1452. https://doi.org/10.1007/s00216-020-03108-3.
- 21) Hanson, A. J.; Maddipatla, D.; Bose, A. K.; Kosik, C. J.; Hajian, S.; Panahi, M.; Masihi, S.; Narakathu, B. B.; Bazuin, B. J.; Atashbar, M. Z. Flexible and Portable Electrochemical System for the Detection of Analytes. In 2021 IEEE International Conference on Flexible and Printable Sensors and Systems (FLEPS); 2021; pp 1–4. https://doi.org/10.1109/FLEPS51544.2021.9469822.
- (22) EmStat Pico Module. PalmSens. https://palmsens.com/product/oem-emstat-pico-module/ (accessed 2021-12-16).
- Jiang, N.; Banerjee, S.; Nilsen-Hamilton, M.; Shrotriya, P. Aptasensor Based on Specific Binding Induced Impedance Changes in Nanoporous Anodized Alumina Membranes. In Chemical, Biological, Radiological, Nuclear, and Explosives (CBRNE) Sensing XXII; SPIE, 2021; Vol. 11749, p 117490H. https://doi.org/10.1117/12.2586170.

3

4

5

6

7

8

9

10

11

12

13

14

15ຊິ

The Gese Anticle, Published and Languer 1903. Rownloaded and 84521 AML.
This afficies is leened under a Creative Commons. Attribution 30 On Borted Lice

44

45

46

47

48

49

50

51

52

53

54

55

56

57

58

59 60 ARTICLE

Journal Name

(24) Chen, Y.-C.; Shan, S.-S.; Liao, Y.-T.; Liao, Y.-C. Bio-Inspired Fractal Textile Device for Rapid Sweat Collection and Monitoring. *Lab on a Chip* **2021**, *21* (13), 2524–2533. https://doi.org/10.1039/D1LC00328C.

- (25) Rowe, A. A.; Bonham, A. J.; White, R. J.; Zimmer, M. P.; Yadgar, R. J.; Hobza, T. M.; Honea, J. W.; Ben-Yaacov, I.; Plaxco, K. W. CheapStat: An Open-Source, "Do-It-Yourself" Potentiostat for Analytical and Educational Applications. PLOS ONE 2011, 6 (9), e23783. https://doi.org/10.1371/journal.pone.0023783.
- (26) Dryden, M. D. M.; Wheeler, A. R. DStat: A Versatile, Open-Source Potentiostat for Electroanalysis and Integration. *PLOS ONE* **2015**, *10* (10), e0140349. https://doi.org/10.1371/journal.pone.0140349.
- (27) Huang, C.-Y.; Syu, M.-J.; Chang, Y.-S.; Chang, C.-H.; Chou, T.-C.; Liu, B.-D. A Portable Potentiostat for the Bilirubin-Specific Sensor Prepared from Molecular Imprinting. *Biosensors and Bioelectronics* 2007, 22 (8), 1694–1699. https://doi.org/10.1016/j.bios.2006.07.036.
- (28) Li, Y. C.; Melenbrink, E. L.; Cordonier, G. J.; Boggs, C.; Khan, A.; Isaac, M. K.; Nkhonjera, L. K.; Bahati, D.; Billinge, S. J.; Haile, S. M.; Kreuter, R. A.; Crable, R. M.; Mallouk, T. E. An Easily Fabricated Low-Cost Potentiostat Coupled with User-Friendly Software for Introducing Students to Electrochemical Reactions and Electroanalytical Techniques. *J. Chem. Educ.* 2018, 95 (9), 1658–1661. https://doi.org/10.1021/acs.jchemed.8b00340.
- (29) Sun, A.; Wambach, T.; Venkatesh, A. G.; Hall, D. A. A Low-Cost Smartphone-Based Electrochemical Biosensor for Point-of-Care Diagnostics. In 2014 IEEE Biomedical Circuits and Systems Conference (BioCAS) Proceedings; 2014; pp 312–315. https://doi.org/10.1109/BioCAS.2014.6981725.
- (30) Cordova-Huaman, A. V.; Jauja-Ccana, V. R.; La Rosa-Toro, A. Low-Cost Smartphone-Controlled Potentiostat Based on Arduino for Teaching Electrochemistry Fundamentals and Applications. *Heliyon* 2021, 7 (2), e06259. https://doi.org/10.1016/j.heliyon.2021.e06259.
- (31) Nemiroski, A.; Christodouleas, D. C.; Hennek, J. W.; Kumar, A. A.; Maxwell, E. J.; Fernández-Abedul, M. T.; Whitesides, G. M. Universal Mobile Electrochemical Detector Designed for Use in Resource-Limited Applications. *PNAS* 2014, 111 (33), 11984–11989. https://doi.org/10.1073/pnas.1405679111.
- (32) Barragan, J. T. C.; Kubota, L. T. Minipotentiostat Controlled by Smartphone on a Micropipette: A Versatile, Portable, Agile and Accurate Tool for Electroanalysis. *Electrochimica Acta* 2020, 341, 136048. https://doi.org/10.1016/j.electacta.2020.136048.
- 33) Mercer, C.; Bennett, R.; Conghaile, P. Ó.; Rusling, J. F.; Leech, D. Glucose Biosensor Based on Open-Source Wireless Microfluidic Potentiostat. Sensors and Actuators B: Chemical 2019, 290, 616–624. https://doi.org/10.1016/j.snb.2019.02.031.
- 34) Krorakai, K.; Klangphukhiew, S.; Kulchat, S.; Patramanon, R. Smartphone-Based NFC Potentiostat for Wireless Electrochemical Sensing. *Applied Sciences* 2021, 11 (1), 392. https://doi.org/10.3390/app11010392.
- (35) Ravindran, S. Smartphone Science: Apps Test and Track Infectious Diseases. *Nature* **2021**, *593* (7858), 302–303. https://doi.org/10.1038/d41586-021-01253-y.
- (36) LMP91000 data sheet, product information and support | TI.com. https://www.ti.com/product/LMP91000 (accessed 2021-12-16).

- (37) mikroC PRO for dsPIC/PIC24 | Mikroe. MikroElektronika Online http://www.mikroe.com/mikroc-dspicpic24 (accessed) 2023) A 12-16).
- (38) EVAL-ADuCM355 Evaluation Board | Analog Devices. https://www.analog.com/en/design-center/evaluation-hardware-and-software/evaluation-boards-kits/EVAL-ADuCM355.html (accessed 2021-12-16).
- (39) AduCM355 examples. https://github.com/analogdevicesinc/aducm355-examples (accessed 2021-07-10).
- (40) ATXMEGA256A3U. https://www.microchip.com/enus/product/ATXMEGA256A3U (accessed 2023-04-05).
- (41) DStat Firmware. DStat firmware. https://microfluidics.utoronto.ca/gitlab/DStat/DStat-firmware (accessed 2023-04-05).
- (42) RN42 | Microchip Technology. https://www.microchip.com/en-us/product/RN42 (accessed 2022-01-29).
- (43) Arduino Mega 2560 Rev3. https://store.arduino.cc/products/arduino-mega-2560-rev3 (accessed 2023-04-05).