

Towards modelling thrombus formation in abdominal aortic aneurysms

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TU/e technische universiteit eindhoven Towards modelling thrombus formation in Abdominal Aortic Aneurysms

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Introduction

In most cases intraluminal thrombus is found in Abdominal Aortic Aneurysms (AAAs), a pathological dilation of the infrarenal aorta (see fig. 1). These blood clots hinder bloodwall transport and alter the mechanical stimulation of endothelial cells, inducing arterial adaptation that can result in aneurysm growth.



Figure 1 Frontal (left) and sagittal (right) view of an AAA with intraluminal thrombus (see arrow). [Courtsey of Leiden University Medical Center, NL]

Thrombus is formed by activation, adhesion and deposition of platelets under influence of various agonists (e.g. APD and Thromboxane III). Mathematically, these processes can be described by a set of coupled convection-diffusion equations (cf. [1]):

$$\frac{\partial c_i}{\partial t} + \boldsymbol{v} \cdot \nabla c_i = D_{iS} \nabla^2 c_i + S_i$$
(1)

with c_i the concentration of the species involved, \vec{v} the velocity, D_{iS} the diffusion coefficient and S_i the source term.

Methods

To obtain the necessary velocity field for eq. (1) we focus on solving the instationary Navier-Stokes equations:

$$\begin{cases} \rho \left(\frac{\partial \boldsymbol{v}}{\partial t} + \boldsymbol{v} \cdot \boldsymbol{\nabla} \boldsymbol{v} \right) - \eta \boldsymbol{\nabla}^2 \boldsymbol{v} + \boldsymbol{\nabla} p = \boldsymbol{0} \\ \boldsymbol{\nabla} \cdot \boldsymbol{v} = 0 \end{cases}$$
(2)

with density ρ , dynamic viscosity η and pressure p. In SEPRAN [2] the validated (discontinuous pressure) 15-pts tetrahedra are used as benchmark to study the performances of the 10pts tetrahedral in a continuous pressure formulation for an AAA geometry based on patient specific imaging data.

Results

In fig. 2 the 15-pts tetrahedron is validated by simulating a Womersley flow. The results of the AAA simulation (peak inlet flow of 6 [l/min], corresponding to $Re_R \approx 750$) are shown in fig. 3. Using the 10-pts tetrahedra the total number of nodal points is reduced by a factor 3. Total computing time /department of biomedical engineering

is reduced significantly (over 10 times) while the results are comparable.



Figure 2 Validation of the 15-pts tetrahedron by comparing the numerical (circles) and analytical (line) results of oscillating flow in a rigid tube with $Q_{max}(t) = 4$ [l/min] at t=0.5 [s].

Discussion

The 10-pts tetrahedron provides a good alternative for the cost-inefficient 15-pts tetrahedral element. Moreover, they can also be used in a pressure-correction method (PCM) i.e. decoupling the continuity and momentum equation. Preliminary tests of oscillating flow in a tube show less CPU-time consumption per time step, but more time steps are needed.



Figure 3 Cross sectional contour planes of the velocity in an AAA at time t = 0.5 [s] for the 15-pts (left) and the 10-pts (right) tetrahedra.

Future work

- Quantify the differences between 10-pts and 15-pts tetrahedron;
- Assessment of the PCM in physically and geometrically complex problems;
- $\hfill\square$ Define model parameters for eq. (1).

References:

- [1] SORENSEN, E.N. Ann. Biomedical Engng vol. 27(4), pp. 449-458, 1999.
- [2] SEPRAN: User manual and standard problems, Ingenieursbureau SEPRA, 2006.