

Article

Low-cost and effective fabrication of biocompatible nanofibers from silk and cellulose-rich materials

Susana Guzman-Puyol, José Alejandro Heredia-Guerrero, Luca Ceseracciu, Hadi Hajiali, Claudio Canale, Alice Scarpellini, Roberto Cingolani, Ilker S. Bayer, Athanassia Athanassiou, and Elisa Mele ACS Biomater. Sci. Eng., Just Accepted Manuscript • DOI: 10.1021/acsbiomaterials.5b00500 • Publication Date (Web): 14 Mar 2016 Downloaded from http://pubs.acs.org on March 15, 2016

Just Accepted

"Just Accepted" manuscripts have been peer-reviewed and accepted for publication. They are posted online prior to technical editing, formatting for publication and author proofing. The American Chemical Society provides "Just Accepted" as a free service to the research community to expedite the dissemination of scientific material as soon as possible after acceptance. "Just Accepted" manuscripts appear in full in PDF format accompanied by an HTML abstract. "Just Accepted" manuscripts have been fully peer reviewed, but should not be considered the official version of record. They are accessible to all readers and citable by the Digital Object Identifier (DOI®). "Just Accepted" is an optional service offered to authors. Therefore, the "Just Accepted" Web site may not include all articles that will be published in the journal. After a manuscript is technically edited and formatted, it will be removed from the "Just Accepted" Web site and published as an ASAP article. Note that technical editing may introduce minor changes to the manuscript text and/or graphics which could affect content, and all legal disclaimers and ethical guidelines that apply to the journal pertain. ACS cannot be held responsible for errors or consequences arising from the use of information contained in these "Just Accepted" manuscripts.



ACS Biomaterials Science & Engineering is published by the American Chemical Society. 1155 Sixteenth Street N.W., Washington, DC 20036 Published by American Chemical Society. Copyright © American Chemical Society. However, no copyright claim is made to original U.S. Government works, or works produced by employees of any Commonwealth realm Crown government in the course of their duties

Page 1 of 32

1	
2	
3	
4	
5	
6	
7	
8	
å	
3	
10	
11	
12	
13	
14	
15	
16	
17	
18	
19	
20	
21	
21 22	
22	
23	
24	
25	
26	
27	
28	
29	
30	
31	
32	
33	
24	
34	
35	
36	
37	
38	
39	
40	
41	
42	
43	
44	
45	
16	
40	
47	
48	
49	
50	
51	
52	
53	
54	
55	
56	
57	
58	
50	
59	

60

Low-cost and effective fabrication of biocompatible nanofibers from 1 silk and cellulose-rich materials 2 3 Susana Guzman-Puyol^{a,*}, José A. Heredia-Guerrero^a, Luca Ceseracciu^a, Hadi Hajiali^{a,b}, Claudio 4 Canale^c, Alice Scarpellini^d, Roberto Cingolani^{a,c,d}, Ilker S. Bayer^a, Athanassia Athanasiou^{a,*}, Elisa 5 Mele $a, \dagger, *$ 6 7 ^a Smart Materials, Istituto Italiano di Tecnologia, Via Morego, 30, Genova, 16163, Italy 8 ^b DIBRIS, University of Genoa, Via Opera Pia, 13, Genova, 16145, Italy 9 ^c Nanophysics, Istituto Italiano di Tecnologia, Via Morego, 30, Genova, 16163, Italy 10 ^d Nanochemistry, Istituto Italiano di Tecnologia, Via Morego, 30, Genova, 16163, Italy 11 12 E-mail addresses: susana.guzman@iit.it, athanassia.athanassiou@iit.it, e.mele2@lboro.ac.uk 13 14 [†] Present address: Department of Materials, Loughborough University, Loughborough, 15 Leicestershire, LE11 3TU, UK 16 17 Abstract 18

Here, we show the production of nanofibrous mats with controlled mechanical properties and excellent biocompatibility by combining fibroin with pure cellulose and cellulose-rich parsley powder agro-waste. To this end, trifluoroacetic acid was used as common solvent for all the involved biomaterials, achieving highly homogeneous blends that were suitable for the electrospinning technique. Morphological analysis revealed that the electrospun composite nanofibers were well-defined and defect-free, with a diameter in the range of 65-100 nm. Mechanical investigations demonstrated that the fibrous mats exhibited an increased stiffness when pure fibroin was combined with cellulose, whereas they possessed an increased flexibility when the parsley waste was added to fibroin. Lastly, the produced mats were highly biocompatible, as demonstrated by the promoted proliferation of fibroblast cells. The characteristics of the hybrid fibroin-cellulose nanofibers, in terms of nanoscale topography, mechanical properties and biocompatibility, are attractive and potentially applicable in the biomedical sector.

32 Introduction

Fibroin and cellulose are two biomaterials often found in natural fibrillary structures because they provide structural support and mechanical resistance that are crucial for the vital functions of insects and plants [1]. In particular, the fibroin microfibrils are structural components of the silk produced by spiders and silkworms [2]. The fibers of the silkworm Bombyx Mori cocoon, for instance, are formed by two filaments of fibroin, held together by a matrix of sericin [3], Figure 1A. The orientation and crystalline structure of the fibroin domains confer to these fibers high mechanical strength and extensibility that is important to provide protection to the silkworm pupae from external threats [4]. On the other hand, in the vegetable kingdom, cellulose microfibrils are the main building blocks of plant cell walls. They are mainly constituted by oriented (1,4)-linked β -D glucan chains that are embedded in a matrix of polysaccharides, such as pectin and hemicelluloses [5], Figure 1B. Cellulose microfibrils are stiff enough to protect plant cells from environmental stresses and to resist to the internal turgor pressure during cell growth and expansion [6].

Page 3 of 32



Figure 1. Schematic of the main components of (A) *Bombyx mori* cocoon and (B) parsley stem residues, and
relative organization at different scales.

The excellent mechanical properties of both fibroin and cellulose materials, together with their biocompatibility and biodegradability, have fostered the development of strategies able to effectively use these two biopolymers to create novel composite systems with applications in different sectors [7,8]. In particular, films with tunable mechanical performances and controlled water stability have been prepared starting from homogeneous ionic-liquid solutions of fibroin and cellulose [9-11]. These films have been used to direct the chondrogenesis of mesenchymal stem cells [10] and to promote the proliferation of fibroblasts [11]. Moreover, other solvents, such as aqueous cuprammonium hydroxide [12-14] and N-methylmorpholine oxide [15], have been use to blend both those biopolymers and to form films. In each case, an interaction between fibroin and cellulose has been observed. Furthermore, microfibers with a diameter ranging between 15 and 40 μ m have been fabricated by wet [16,17] and dry spinning [18,19] of fibroin-cellulose blends. On the contrary, to the best of our knowledge, to date no attempts have been reported on the production of

fibroin-cellulose blend nanofibers (diameter in the submicron range), despite the increasingattention that these nanostructures are gaining in regenerative medicine [20].

A technology that is of particular interest for this research area is electrostatic spinning (ES), because it allows to fabricate nanofibrous mats and scaffolds with the desired biophysical, biochemical and biomechanical properties [21]. The nanoscale topography and the three-dimensional (3D) interconnected porosity of the electrospun constructs have been used to control cell proliferation, migration and differentiation [22,23]. Furthermore, a variety of biocompatible and biodegradable, synthetic and natural materials can be processed by ES, including fibroin [24-27]. In fact, electrospun nanofibers of this protein and its combination with other biopolymers, such as poly(ethylene oxide), poly(L-lactic acid-co- ε -caprolactone), chitosan, and collagen, have been proposed for the regeneration of blood vessels and nerves [28,29]. Previous works on ES of fibroin have reported the use of water, ionic liquids, hexafluoroisopropanol or hexafluoroacetone hydrate as solvents [30-33].

In this paper, we show that hybrid nanofibers of fibroin (from *Bombyx mori* silkworm cocoons) and microcrystalline cellulose or cellulose-rich parsley waste can be electrospun using trifluoroacetic acid (TFA) as common solvent, without the need of additives or subsequent treatments. In particular, mats of well-defined and defect-free nanofibers were produced by combining fibroin with pure cellulose or dried powder of parsley (*Petroselinum crispum*) stems at a 1:1 ratio. The physicochemical characterization of the samples revealed that the different constituents were well distributed inside the nanofibers without segregation or phase separation effects. The addition of cellulose to fibroin allowed the production of stiffer mats. Interestingly, nanofibers containing parsley exhibited an elastic modulus comparable to that of the fibroin fibers but with a higher elongation at maximum load. Furthermore, all the nanofibrous supports were highly biocompatible, promoting the adhesion and proliferation of fibroblasts. The use of dried parsley stems as source of cellulose demonstrated that valuable products can be obtained even from vegetable waste, rich in cellulose, through the here discussed procedure. Furthermore, *Petroselinum crispum* is an herb of

87 interest for biomedical applications, because it contains bioactive compounds, including
88 antioxidants, anticancer and anti-inflammatory molecules [34-36].

90 Materials and methods

91 Materials and cell line

Bombyx mori silkworm cocoons used in this research were purchased from Angkorchum Trading Inc. In order to remove sericin, raw silk was degummed using a 0.02 M solution of Na₂CO₃ in boiling water for 30 minutes. Degummed silk fibers were then washed thoroughly with deionized water to remove any remaining sericin and rest of surfactants, and then dried in air overnight. After degumming and drying, raw silk lost about 25% of its original weight. High purity microcrystalline cellulose (MCC, crystallinity ~79%) from cotton linters and anhydrous TFA were purchased from Sigma Aldrich and used as received. Dried powder of parsley (*Petroselinum crispum*) stems was provided by a vegetable producer (Ida S.r.l., Italy) as not edible food waste.

For the biocompatibility assay, Dulbecco's Modified Eagle's Medium (DMEM), Bovine Calf Serum
(BCS), trypsin–EDTA solution, penicillin-streptomycin, Phosphate Buffered Saline (PBS),
fuoroshield with DAPI and thiazolyl blue tetrazolium bromide (MTT) were purchased from Sigma
Aldrich. Alexa Fluor® 488 phalloidin was from Life Technology. Fibroblast cells from murine
embryo (NIH3T3-cells) were obtained from ATCC® (CRL-1658TM).

106 Fabrication of the electrospun nanofibers

107 Solutions for electrospinning were prepared by separately dissolving fibroin, MCC and dried 108 parsley powder in TFA at a concentration of 3% w/w. The procedure described in Ref. [37] was 109 followed for cellulose and parsley solutions. Briefly, cellulose solutions were obtained by 110 dissolving MCC in TFA for 3 days under shaking, whereas the dissolution of pulverized parsley 111 stems took 28 days under shaking, and of fibroin just few seconds. Then, the fibroin solution was

mixed with the MCC or the parsley solution at 1:1 volume ratio, in order to have MCC: fibroin or parsley:fibroin blends, respectively. Other combinations of MCC:fibroin and parsley:fibroin were also prepared but they were not suitable for the ES process producing particles instead of fibers or fibers with a high number of beads. For this reason we selected the combination 1:1 volume ratio. For the ES process, a syringe with a stainless-steel 23-gauge needle was filled with the polymer solution (fibroin, MCC:fibroin or parsley:fibroin) and connected to a syringe pump (NE-1000, New Era Pump Systems, Inc.) working at a constant flow rate of 1 mL/hour. The needle was clamped to the positive electrode of a high-voltage power supply generating 18 kV, and an aluminum disk (diameter 50 mm, thickness 3 mm) rotating at a speed of 2500 rpm was used as collector (needlecollector distance of 15 cm). The ES experiments were conducted by means of the high speed roto-translating electrospinning system of Linari Engineering (RT Collector Web).

Morphological characterization

High-resolution Scanning Electron Microscopy (SEM) imaging was carried out using a JEOL JSM 7500FA (Jeol, Tokyo, Japan) equipped with a cold field-emission gun (FEG), operating at 15 kV acceleration voltage. The samples were coated with a 10 nm thick film of carbon using an Emitech K950X high vacuum turbo system (Quorum Technologies Ltd, East Sussex - UK). Imaging was performed with the secondary electrons to analyze the morphology of the fibers. The fibers' diameter was calculated with ImageJ image analyzer program. Basically, the SEM images were loaded into the software and diameter of the fibers was measured using a two point measuring analysis. Approximately, 100 measurements were taken to obtain the diameter distribution of each type of fibers.

Chemical and structural characterization

Infrared spectra were obtained with an Attenuated Total Reflectance (ATR) accessory (MIRacle ATR, PIKE Technologies) coupled to a Fourier Transform Infrared (FTIR) spectrometer (Equinox

70 FT-IR, Bruker). All spectra were recorded in the range from 4000 to 600 cm⁻¹ with a resolution of 4 cm⁻¹, accumulating 128 scans. Measurements were performed on nanofibers of fibroin, MCC: fibroin and parsley: fibroin, and on films of cellulose and parsley after treatment with TFA. To assess the homogeneity of chemical composition, ATR-FTIR spectra were recorded three times on different samples. Deconvolution of amide I components (1720-1580 cm⁻¹) was carried out by using of PeakFit 4.11 software. In order to remove the contribution of cellulose or parsley in this spectral region, spectra of such components were subtracted by the mixtures' spectra by previous normalization respect to C-O stretching of polysaccharides (ca. 1016 cm⁻¹ for cellulose and 1022 cm⁻¹ for parsley). Wavenumber positions of components were deduced by calculation of the second-order derivative. Deconvolution was performed using Gaussian shape with an amplitude threshold of 3%. A non-linear least-square method was employed to reduce the differences between the calculated spectra and the original one. The crystalline structure of nanofibers was analyzed by X-ray diffraction (XRD) using a diffractometer Rigaku SmartLab X-Ray Diffractometer equipped with a copper rotating anode. The X-ray source was operated at 40 kV and 150 mA. A Gobel mirror was used to obtain a parallel beam and to suppress Cu K β radiation (1.392 Å). The measurements were performed using a 2θ scan.

155 Thermal characterization

The thermal degradation behavior of the nanofibers was investigated by a standard thermogravimetric analysis (TGA) method using a TGA Q500 from TA Instruments. Measurements were performed on 3-5 mg of samples in an aluminum pan under inert N_2 atmosphere with a flow rate of 50 mL/min at a temperature range from 30 to 600°C and a heating rate of 5°C/min. The weight loss and its first derivative were recorded simultaneously as a function of time/temperature.

162 Mechanical characterization

The mechanical properties of mats were obtained by uniaxial tension tests on a dual column universal testing machine (Instron 3365). Mats were cut in prismatic specimen with a width of 4 mm and an effective length of 25 mm. In order to avoid accidental damage during handling, specimens were tested with the paper frame method, already reported in Ref. [38]; briefly, the samples were first taped on custom made paper frames composed by two detachable halves, then mounted on the testing machine's hydraulic clamps. Displacement was applied with the rate of 2 mm/min. From the resulting stress strain curves, the apparent elastic modulus, ultimate tensile strength (UTS), elongation at yield and elongation at maximum load were extracted. The term "apparent" refers to the fact that the measured value is not an intrinsic property of the bulk material, but depends on the mat density and structure. Measurements were performed on 5 samples per each material. All the stress-strain curves were recorded at 25 °C and 44% relative humidity (RH). Single-fiber mechanical characterization was performed in a liquid environment of phosphate-buffered saline (PBS) by atomic force microscope (AFM) by a Nanowizard III (JPK Instruments, Germany) mounted on an Axio Observer D1 (Carl Zeiss, Germany) inverted optical microscope. V-shaped DNP silicon nitride cantilevers (Bruker, Massachussets, US) with a nominal spring constant 0.24 N/m, resonance frequency in air ranging from 40 kHz to 75 kHz and tip typical curvature radius of >20 nm were used. The actual spring constant of each cantilever was determined *in situ* using the thermal noise method [39]. Images were acquired in quantitative imaging (QI) mode, a recently developed imaging mode based on force measurements [40]. A maximum force of 7 nN was applied on the sample and 256×256 force-distance (FD) curves were acquired per each image. Then, FD curves were converted into force-indentation (FI) and the stiffness was extracted from the curves slope. **Biocompatibility study**

NIH3T3 cells were cultured in DMEM supplemented with 10% of BCS and 1% of antibiotics (100 U/mL penicillin and 0.1 mg/mL streptomycin), in incubator at 37 °C with 5% CO₂. The culture

medium was replaced every 3 days. The electrospun samples were sterilized under ultraviolet (UV) light for 30 minutes, and subsequently they were washed using a PBS solution. Fibroblast cells were detached from the culture flask using trypsin-EDTA solution, when 80% of confluence was reached, and seeded onto the electrospun mats. Adhered and proliferated cells, cultured for 24 hours, were analysed by a colorimetric MTT assay. In order to observe the morphology of cells, the samples were fixed in 3.7% formaldehyde for 15 min before rinsing them with PBS for 3 times. Samples were then permeabilized with 1% Triton X-100, and stained with alexa-fluor 488 phalloidin and DAPI for actin cytoskeleton and nucleus, respectively. The confocal microscope Nikon A1 was utilized to visualize the morphology of fluorescent-stained 3T3 fibroblasts on the electrospun fibres.

Results and discussion

201 Morphological characterization

The SEM images in Figure 2A show that electrospinning fibroin from TFA solutions resulted in well-defined nanofibers without defects or beads. The analysis of the fiber population in the mat demonstrated a predominance of fibers having a size in the range of 50-120 nm (72% of the total population, Figure 2D). The calculated average diameter was of (103±25) nm. When fibroin solution was blended with MCC or parsley waste solution (1:1 ratio), the use of TFA as common solvent promoted the miscibility of the polymers, without inducing phase separation before the ES process. This positively affected the morphology of the produced composite fibers that were free from beaded structures, as visible in Figure 2B and 2C for MCC:fibroin and parsley:fibroin, respectively. In both cases, the average diameter of the fibers decreased of about 37% with respect to pure fibroin, being (65 ± 11) nm and (64 ± 12) nm for MCC: fibroin (Figure 2E) and parsley: fibroin (Figure 2F) nanofibers, respectively. The majority of the population (approximately 70%) was characterized by a size in the range of 50-70 nm, and no fibers had a diameter larger than 180 nm.



219

220



Figure 2. SEM images of the electrospun nanofibers: (A) fibroin, (B) MCC:fibroin and (C) parsley:fibroin.
Histograms showing the width distribution of the nanofibers: (D) fibroin, (E) MCC:fibroin and (F) parsley:fibroin.

221 Chemical, structural and thermal characterization

The chemical characterization of fibroin, MCC:fibroin, and parsley:fibroin nanofibers was carried out by ATR-FTIR. As shown in Figure 3A, the samples are characterized by the presence of vibrations associated with fibroin (amide A –hydrogen-bonded NH stretching– at 3279 cm⁻¹, amide B –NH Fermi resonance– at 3074 cm⁻¹, amide I –C=O stretching– at 1640 cm⁻¹, amide II –in-plane N-H bending coupled to C-N stretching– at 1515 cm⁻¹, and amide III –similarly to amide II, inplane N-H bending coupled to C-N stretching– at 1236 cm⁻¹) [41,42]. Moreover, characteristic bands of cellulose (OH stretching at 3354 cm⁻¹, CH stretching at 2889 cm⁻¹, adsorbed water at 1643

cm⁻¹, ring breathing at 1155 cm⁻¹, and C-O stretching at 1016 cm⁻¹) [43] or parsley (OH stretching at 3294 cm⁻¹, asymmetric and symmetric CH₂ stretching of lipid molecules at 2918 and 2851 cm⁻¹, respectively, C=C stretching of lignin at 1672 cm⁻¹, and C-O stretching of polysaccharides at 1022 cm⁻¹) [37] can be observed. No traces of TFA were detected. However, small modifications of the shape of amide I and II absorptions in the spectra of MCC:fibroin and parsley:fibroin samples with respect to the fibroin one were observed. Usually, such differences are ascribed to changes of the secondary structure of the fibroin that were quantified by deconvolution of amide I vibration [44], Figure 3B. Amide I components are shown in Figure S1 (supplementary information). For fibroin nanofibers main contribution was associated with random coils, while β -sheets and turns were lightly smaller. Minor fractions were side chains and α -helices. These results are consistent with Ha et al. (2006) [45] who stated that regenerated fibroin from TFA solutions shows random coil and β sheet characteristics. In the case of MCC:fibroin also random coil was the main component and turns and α -helices increased their values at the expense of β -sheets and side chains, while parsley: fibroin sample presented a pattern of contributions very similar to pure fibroin.



Figure 3. (A) ATR-FTIR spectra of the electrospun nanofibers. (B) Contribution to amide (%) from
deconvolution of the amide I region of the ATR-FTIR spectra. (C) XRD patterns of the electrospun
nanofibers. (D) TGA thermograms and derivative thermogravimetric curves of the electrospun nanofibers.

The diffractograms in Figure 3C displayed a broad halo centered around 20-21° for all types of nanofibers. This can be ascribed to a strong amorphous character of cellulose or parsley components after TFA treatment [37], according with ATR-FTIR data but also to the amorphous contribution of silk fibroin [46].

The thermal properties of fibroin, MCC:fibroin and parsley:fibroin nanofibers were examined by TGA. TGA thermograms and the corresponding derivative curves are shown in Figure 3D top and bottom, respectively. A region of weight loss for temperature values up to 100 °C was observed for all the samples and it was due to the loss of water (environmental humidity) absorbed by the electrospun mats. Fibroin nanofibers (red curve) exhibited a second region of weight loss between 270 and 380 °C with a peak at 274 °C that was associated with the degradation of amino acid side groups and cleavage of peptide bonds [47,48]. On the other hand, MCC: fibroin nanofibers (grey curve) showed two main thermal events at 280 and 316 °C, being ascribed to the degradation of fibroin and cellulose fraction, respectively. In fact, pure cellulose films prepared using TFA as solvent present a single well-defined thermal degradation peak at 326 °C [37]. Finally, the thermogram of parsley: fibroin nanofibers (green curve) was characterized by three main peaks at 157, 217 and 271 °C. The first two peaks can be attributed to the parsley fraction, whereas the third peak is related to the juxtaposition of the main degradation peaks of fibroin and parsley. As previously reported in literature, bioplastics prepared from parsley stem residues have a first weight loss at 144 °C, a second at 219 °C, and a third one at 277 °C, ascribed to the existence of diverse organic components [37].

270 Mechanical characterization

ACS Biomaterials Science & Engineering

Typical stress-strain curves of each type of nanofibers are reported in Figure 4A. Two different behaviors can be noticed: fibroin and MCC:fibroin mats present a short slack recovery, followed by a classical Hookean linear deformation, and by yield and plastic deformation. Parsley:fibroin samples, instead, exhibit a nonlinear deformation behavior with an initial large deformation at low load, followed by a quick increment of stiffness. The elastic modulus, ultimate tensile strength (UTS), strain at yield and elongation at maximum load extracted from such curves are reported in Table 1 and in Figure 4B. For parsley:fibroin nanofibers, the elastic moduli associated with both regions are reported.



Figure 4. (A) Stress-strain curves of the electrospun nanofibers. Inset: photograph of the nanofibers just after the electrospinning process. (B) Mechanical parameters for the electrospun nanofibers calculated from the stress-strain curves. For parsley:fibroin sample, the two values of elastic modulus corresponding to the two different mechanical behaviors are indicated. (C) Elongation versus elastic modulus data and (D) ultimate tensile strength versus elastic modulus data where other nanofibers prepared using electrospinning are showed.

Sample	Apparent elastic modulus (MPa)	Ultimate tensile strength (MPa)	Elongation at yield (%)	Elongation at maximum load (%)
Fibroin	125±21	5.8±0.2	5.5±1.2	10.6±1.7
MCC:fibroin	293±56	6.4±1.2	2.9±0.3	3.4±0.5
Parsley:fibroin	22±11 108±21	4.3±0.9	8.1±2.1	8.1±2.1

Table 1. Mechanical properties (apparent elastic modulus, ultimate tensile strength, elongation at yield and elongation at maximum load) of nanofibers. Data are expressed as mean \pm s.d. (n \geq 5). For parsley:fibroin sample, the two values of elastic modulus corresponding to the two different mechanical behaviors are indicated.

The obtained stress strain curves can be explained by considering the compositional and morphological differences of the studied materials. The mechanical behavior of pure fibroin mats and their apparent elastic modulus of (125 ± 21) MPa are consistent with previous reports in literature [48]. When fibroin was combined with cellulose a change in the stiffness of the mat was observed, with an increment of the elastic modulus that reached (293±56) MPa for MCC:fibroin nanofibers. Moreover, the strain at yield of the MCC: fibroin samples was lower (\sim 3%) than that one of fibroin sample (\sim 5%); similarly, the elongation at maximum load was negatively affected by the presence of cellulose, with values lower for MCC: fibroin mats ($\sim 3\%$) than for pure fibroin ($\sim 11\%$). It should be noted that the strength was not reduced, suggesting a good mixing of both components. In the case of the parsley: fibroin mats, it is worth noting that their nonlinear behavior is similar to the one of human tendons [49]. For those natural structures, it can be attributed to a crimped waveform organization of the fibers, which is confirmed also for the parsley: fibroin fibers by SEM observations as seen in Figure S2 (supplementary information). The first, low stiffness region, corresponded to the uncoiling of the crimps, enhanced by the low modulus and high flexibility of

ACS Biomaterials Science & Engineering

parsley-based material, as already presented in Ref. [37]. The second region behavior most likely
starts when most fiber strands are aligned and is mainly ruled by the stiffness of fibroin. The elastic
modulus reached a value of (108±21) MPa and the fibers were characterized by a strain at yield of
about 8%.

A comparison of the mechanical properties of the measured samples with those of other electrospun materials is shown in Figures 4C and 4D [50-56]. Although the effect of the fiber network morphology should be considered for a direct comparison, yet it is possible to appreciate that our blends have a similar stiffness to the one of other natural-based materials, such as fibroin [50] and collagen [51] and comparable values of UTS and elongation of common polymer fibers, such as poly(methyl methacrylate) (PMMA) [52], polyvinyl chloride (PVC) [53], polycaprolactone (PCL) [54] and polyurethane (PU) [53].

Considering silk composites, the addition of cellulose has a similar effect, in relative terms, as the addition of single-wall nanotubes (SWNT) in a narrow concentration range [57]. An additional comparison can be made with composites, not produced by electrospinning, based on combinations of fibroin and cellulose (or other polysaccharides), although the sample structure strongly affects the absolute values of mechanical properties. The general modification induced by the addition of cellulose to fibroin is an increment in elongation as well as, to a lesser extent, in strength, while stiffness is usually unaffected [3,12,16,17]. We have, on the contrary, higher stiffness and strength, but a reduction of the tenacity and elongation. We attribute this to the characteristics of MCC obtained through our treatment, stiffer than the one processed by different routes [16, 37, 58]. Therefore, when added to fibroin, it acts as reinforcement rather than plasticizer.

In order to investigate the structural homogeneity of the produced nanofibers, AFM nanoindentation analysis was conducted in PBS medium (Figure 5). The local stiffness was chosen for such characterization, as it is more sensitive than topology to differentiate different phases even in absence of morphological difference. The maps of the stiffness shown in Figure 5 indicated a homogenous and narrow distribution of values in both pure fibroin and hybrid nanofibers, without evident subdomains. This indicates the lack of segregation of the different components and confirms the well mixing and blending for MCC:fibroin and parsley:fibroin nanofibers. The values of stiffness are in agreement with the trend previously discussed for the mats (Figure 4).



Figure 5. AFM mappings of the electrospun nanofibers showing the indentation stiffness of fibroin,
 MCC:fibroin and parsley:fibroin nanofibers. The map homogeneity indicates good mixing of the
 components.

Biocompatibility assays

 The biocompatibility of the electrospun mats was evaluated using fibroblast cells as *in-vitro* model. Figure 6A shows the MTT results of cell proliferation after 24 hours for the different nanofibrous samples and control (glass substrate). All the prepared nanofibers (pure fibroin, MCC:fibroin and parsley:fibroin) exhibited excellent cell compatibility (higher than the control) and no cytotoxic effects. This verifies that the use of TFA was not detrimental for the cells. Indeed, the acid completely evaporated during the ES process, as demonstrated by ATR-FTIR spectroscopy (Figure 3A). Morphological analysis pointed out that the fibroblast cells attached well and spread on the

ACS Biomaterials Science & Engineering

electrospun mats nanofibers (Figure 6B-6G). This is also due to the nanometric size of the fibers and their 3D organization that both promote cell proliferation by mimicking the fibrillary topography and high surface area of the native extracellular matrix (ECM) [28]. It is important also to be considered that, in general terms, the chemical composition of the here developed composite fibers of protein and polysaccharide recalls the one of ECM. In fact, in tissues and organs, ECM is a combination of several molecules including proteins (such as collagen and elastin), polysaccharides (such as hyaluronan and chondroitins), proteoglycans, and adhesive glycoproteins [59]. в Α 160-Cell proliferation (%)



D

Figure 6. Viability of fibroblast cells (MTT assay) on the different types of nanofibers. Mean \pm standard deviation (n = 3) (A). Fluorescence micrographs of fibroblast cells cultured on (B, E) fibroin, (D, F) MCC: fibroin and (D, G) parsley: fibroin nanofibers.

Parsley:fibroin

MCC:fibroin

Fibroin

Conclusions

Control

In conclusion, we used TFA to codissolve fibroin and cellulose-based materials (pure cellulose and dried powder of parsley stem residues) and to produce hybrid nanofibers (MCC:fibroin and parsley: fibroin) by electrospinning. The choice of TFA as single solvent allowed us to prepare highly mixed blends and, consequently, to avoid phase separation effects in the final nanofibers, as confirmed by morphological and mechanical analysis. In particular, AFM nanoindentation tests demonstrated a uniform distribution of the diverse components inside the nanofibers, without the

presence of domains having different properties. No cytotoxic byproducts were formed due to the use of TFA, allowing applying the electrospun mats as scaffolds for promoting the proliferation of fibroblast cells. Especially, parsley: fibroin mats showed excellent biocompatibility, probably due to the proper combination of nanoscale topography and mechanical flexibility. The here-discussed method for blending together fibroin and cellulose-based materials and for processing them by ES can be extended to other naturally-derived polymers, creating novel systems for biomedical applications. Moreover, the possibility to process vegetable residues containing cellulose is attractive in view of the valorization and sustainable management of food waste.

380 Supplementary information

Deconvolution of amide I absorption for fibroin, MCC:fibroin, and parsley:fibroin nanofibers and SEM image of parsley:fibroin nanofibers. This material is free of charge via the Internet at <u>http://pubs.acs.org</u>.

385 Notes

386 The authors declare no competing financial interest.

388 Acknowledgements

The authors thank to Mrs. Lara Marini for her assistance with the thermal measurements and Dr. Giovanni Perotto for his helpful comments and recommendations. J. A. Heredia-Guerrero acknowledges the BIOPROTO project (Marie Curie Intra-European Fellowship), financed by the EU Seventh Framework Programme for Research (FP7). Authors also thank to A. Gemma (Ida S.r.l.) for providing the parsley waste.

References

3	396	[1] Fratzl, P.; Weinkamer, R. Nature's hierarchical materials. Progress in Materials Science 2007,
4 5 6	397	52, 1263-1334.
0 7 8	398	[2] Xu, M; Lewis, R.V. Structure of a protein superfiber: Spider dragline silk. Proc. Natl. Acad. Sci.
9 10	399	<i>USA</i> 1990 , <i>87</i> , 7120-7124.
11 12	400	[3] Ude, A.U.; Eshkoor, R.A.; Zulkifili, R.; Ariffin, A.K.; Dzuraidah, A.W.; Azhari, C.H. Bombyx
13 14 15	401	mori silk fibre and its composite: A review of contemporary developments. Materials and Design
16 17	402	2014 , <i>57</i> , 298-305.
18 19	403	[4] Chen, F.; Porter, D.; Vollrath, F. Structure and physical properties of silkworm cocoons. J. R.
20 21	404	Soc. Interface 2012, 9, 2299-2308.
22 23	405	[5] Cosgrove, D.J. Growth of the plant cell wall. Nature Reviews 2005, 6, 850-861.
24 25 26	406	[6] Marga, F.; Grandbois, M.; Cosgrove, D.J.; Baskin, T.I. Cell wall extension results in the
27 28	407	coordinate separation of parallel microfibrils: evidence from scanning electron microscopy and
29 30	408	atomic force microscopy. The Plant Journal 2005, 43, 181-190.
31 32	409	[7] Bledzki, A.K.; Gassan, J. Composites reinforced with cellulose based fibres. Prog. Polym. Sci.
33 34 25	410	1999 , <i>24</i> , 221-274.
35 36 37	411	[8] Hardy, J.G.; Scheibel, T.R. Composite materials based on silk proteins. Prog. Polym. Sci.
38 39	412	2010 , <i>35</i> , 1093-1115.
40 41	413	[9] Shang, S.; Zhu, L.; Fan, J. Physical properties of silk fibroin/cellulose blend films regenerated
42 43	414	from the hydrophilic ionic liquid. Carbohyd. Polym. 2011, 86, 462-468.
44 45 46	415	[10] Singh, N.; Rahatekar, S.S.; Koziol, K.K.K.; Ng, T.H.S.; Patil, A.J.; Mann, S.; Hollander, A.P.;
40 47 48	416	Kafienah, W. Directing Chondrogenesis of Stem Cells with Specific Blends of Cellulose and Silk.
49 50	417	<i>Biomacromolecules</i> 2013 , <i>14</i> , 1287-1298.
51 52	418	[11] Zhou, L.; Wang, Q.; Wen, J.; Chen, X. Shao, Z. Preparation and characterization of transparent
53 54	419	silk fibroin/cellulose blend films. Polymer 2013, 54, 5035-5042.
55 56 57		
58 59		
60		19

[12] Freddi, G.; Romanò, M.; Massafra, M.R.; Tsukada, M. Silk fibroin/cellulose blend films:
preparation, structure, and physical properties. *Journal of applied polymer science* 1995, *56*, 15371545.

- 423 [13] Yang, G.; Zhang, L.; Liu, Y. Structure and microporous formation of cellulose/silk fibroin
 424 blend membranes: I. Effect of coagulants. *Journal of membrane science* 2000, *177*, 153-161.
- 425 [14] Yang, G.; Zhang, L.; Cao, X.; Liu, Y. Structure and microporous formation of cellulose/silk
 426 fibroin blend membranes: Part II. Effect of post-treatment by alkali. *Journal of membrane science*427 2002, *210*, 379-387.
- 428 [15] Sashina, E.; Janowska, G.; Zaborski, M.; Vnuchkin, A. Compatibility of fibroin/chitosan and
 429 fibroin/cellulose blends studied by thermal analysis. *Journal of Thermal Analysis and Calorimetry*430 2007, *89*, 887-891.
- 431 [16] Hirano, S.; Nakahira, T.; Zhang, M.; Nakagawa, M.; Yoshikawa, M.; Midorikawa, T. Wet432 spun blend biofibers of cellulose-silk fibroin and cellulose-chitin-silk fibroin. *Carbohyd. Polym.*433 2002, 47, 121-124.
- 434 [17] Marsano, E.; Canetti, M.; Conio, G.; Corsini, P.; Freddi, G. Fibers Based on Cellulose-Silk
 435 Fibroin Blend. *J. Appli. Polym. Sci.* 2007, *104*, 2187-2196.
- 436 [18] Yao, Y.; Zhang, E.; Xia, X.; Yu, J.; Wu, K.; Zhang, Y.; Wang, H. Morphology and properties
- 437 of cellulose/silk fibroin blend fiber prepared with 1-butyl-3-methylimidazolium chloride as solvent.
- *Cellulose* **2015**, *22*, 625-635.
 - 439 [19] Marsano, E.; Corsini, P.; Canetti, M.; Freddi, G. Regenerated cellulose-silk fibroin blends
 440 fibers. *Int. J. Biol. Macromol.* 2008, *43*, 106-114.
 - [20] Zhang, L.; Webster, T.J. Nanotechnology and nanomaterials: Promises for improved tissue
 regeneration. *Nano Today* 2009, *4*, 66-80.
 - 443 [21] Braghirolli, D.I.; Steffens, D.; Pranke, P. Electrospinning for regenerative medicine: a review
 - 444 of the main topics. *Drug Discov. Today* **2014**, *19*, 743-753.

3
1
4 F
5
6
7
8
9
10
11
11
12
13
14
15
16
17
18
10
10
20
21
22
23
24
25
26
20
20
28
29
30
31
32
33
34
35
20
30
37
38
39
40
41
42
12
43
44
40
46
47
48
49
50
51
50
52
53
54
55
56
57
58
59

60

445 [22] Wang, X.; Ding, B.; Li, B. Biomimetic electrospun nanofibrous structures for tissue
446 engineering. *Mater. Today* 2013, *16*, 229-241.

- 447 [23] Pelipenko, J.; Kocbek, P.; Govedarica, B.; Rošic, R.; Baumgartner, S.; Kristl, J. The
- topography of electrospun nanofibers and its impact on the growth and mobility of keratinocytes.
- 449 Eur. J. Pharm. Biopharm. 2013, 84, 401-411.
- 450 [24] Liu, W.; Thomopoulos, S.; Xia, Y. Electrospun Nanofibers for Regenerative Medicine. *Adv.*451 *Healthc. Mater.* 2012, *11*, 10-25.
- 452 [25] Khan, F.; Ahmad, S.R. Polysaccharides and Their Derivatives for Versatile Tissue Engineering
 453 Application. *Macromol. Biosci.* 2013, *13*, 395-421.
- 454 [26] Hajiali, H.; Heredia-Guerrero, J.A.; Liakos, I.; Athanassiou, A.; Mele, E. Alginate nanofibrous
 455 mats with adjustable degradation rate for regenerative medicine. *Biomacromolecules* 2014, *16*, 936456 943.
- 457 [27] Liakos, I.; Rizzello, L.; Hajiali, H.; Brunetti, V.; Carzino, R.; Pompa, P.P.; Athanassiou, A.;
 458 Mele, E. Fibrous wound dressings encapsulating essential oils as natural antimicrobial agents. J.
- 459 *Mater. Chem. B* **2015**, *3*, 1583-1589.
- 460 [28] Zhang, X.; Reagan, M.R.; Kaplan, D.L. Electrospun silk biomaterial scaffolds for regenerative
 461 medicine. *Adv. Drug Deliver. Rev.* 2009, *61*, 988-1006.
- 462 [29] Kundu, B.; Rajkhowa, R.; Kundu, S.C.; Wang, X. Silk fibroin biomaterials for tissue
 463 regenerations. *Adv. Drug Deliver. Rev.* 2013, *65*, 457-470.
- 464 [30] Hodgkinson, T.; Chen, Y.; Bayat, A.; Yuan, X.F. Rheology and Electrospinning of
 465 Regenerated Bombyx mori Silk Fibroin Aqueous Solutions. *Biomacromolecules* 2014, *15*, 1288466 1298.
- 467 [31] Jiang, N.; Huang, X.; Li, Z.; Song, L.; Wang, H.; Xu, Y.; Saho, H.; Zhang, Y. Silk fibroin
 468 tissue engineering scaffolds with aligned electrospun fibers in multiple layers. *RSC Adv.* 2014, *4*,
- **469 47570-47575**.

470 [32] Jin, H.J.; Fridrikh, S.V.; Rutledge, G.C.; Kaplan, D.L. Electrospinning Bombyx mori silk with

- 471 poly (ethylene oxide). *Biomacromolecules* **2002**, *3*, 1233-1239.
- 472 [33] Yao, J.; Masuda, H.; Zhao, C.; Asakura, T. Artificial Spinning and Characterization of Silk
- 473 Fiber from Bombyx m ori Silk Fibroin in Hexafluoroacetone Hydrate. *Macromolecules* 2002, *35*, 6474 9.
- 475 [34] Kaefer, C.M.; Milner, J.A. The role of herbs and spices in cancer prevention. *J. Nutr. Biochem.*476 2008, *19*, 347-361.
- 477 [35] Luthria, D.L. Influence of experimental conditions on the extraction of phenolic compounds
 478 from parsley (Petroselinum crispum) flakes using a pressurized liquid extractor. *Food Chem.*479 2008, 107, 745-752.
- 480 [36] Kuriyama, I.; Musumi, K.; Yonezawa, Y.; Takemura, M.; Maeda, N.; Iijima, H.; Hada, T.;
- 481 Yoshida, H.; Mizushina, Y. Inhibitory effects of glycolipids fraction from spinach on mammalian
- 482 DNA polymerase activity and human cancer cell proliferation. J. Nutr. Biochem. 2005, 16, 594-601.
- 483 [37] Bayer, I.S.; Guzman-Puyol, S.; Heredia-Guerrero, J.A.; Ceseracciu, L.; Pignatelli, F.; Ruffilli,
- 484 R.; Cingolani, R.; Athanassiou, A. Direct Transformation of Edible Vegetable Waste into
- 485 Bioplastics. *Macromolecules* **2014**, *47*, 5135-5143.
- 486 [38] Romano, I.; Mele, E.; Heredia-Guerrero, J.A.; Ceseracciu, L.; Hajiali, H.; Goldoni, L.; Marini,
- 487 L.; Athanassiou, A. Photo-polymerisable electrospun fibres of N-methacrylate glycol chitosan for
 488 biomedical applications. *RSC Adv.* 2015, *31*, 24723-24728.
- 489 [39] Hutter, J.L.; Bechhoefer, J. Calibration of Atomic-Force Microscope tips. *Rev. Sci. Instrum.*490 1993, *64*, 1868-1873.
- 491 [40] Seguezza, S.; Dante, S.; Diaspro, A.; Canale C. High resolution nanomechanical
 492 characterization of multi-domain model membranes by fast Force Volume. *J. Mol. Recog.* 2015.
 493 DOI: 10.1002/jmr.2490.
- 494 [41] Goormaghtigh, E.; Cabiaux, V.; Ruysschaert, J.M. Determination of Soluble and Membrane
 495 Protein Structure by Fourier Transform Infrared Spectroscopy. In *Physicochemical Methods in the*

2
3
4
5
6
7
8
0
9
10
11
12
13
14
15
16
10
17
18
19
20
21
22
23
24
24
25
26
27
28
29
30
31
22
3Z
33
34
35
36
37
38
20
39
40
41
42
43
44
45
46
47
71 10
40
49
50
51
52
53
54
55
55
56
57
58
59
60

496 Study of Biomembranes Subcellular Biochemistry; Hilderson, H.J.; Ralston, G.B., Eds.; Springer,
497 US, 1994; p 329.

- 498 [42] Sionkowska, A.; Planecka, A. Preparation and characterization of silk fibroin/chitosan
 499 composite sponges for tissue engineering. *J. Mol. Liq.* 2013, *178*, 5-14.
- 500 [43] Garside, P.; Wyeth, P. Identification of cellulosic fibres by FTIR spectroscopy Thread and
- 501 single fibre analysis by attenuated total reflectance. *Stud. Conserv.* **2003**, *48*, 269-275.
- 502 [44] Hu, X.; Kaplan, D.; Cebe, P. Determining beta-sheet crystallinity in fibrous proteins by thermal
 503 analysis and infrared spectroscopy. *Macromolecules* 2006, *39*, 6161-6170.
- [45] Ha, S. W.; Tonelli, A.E.; Hudson, S.M. Structural studies of Bombyx mori silk fibroin during
 regeneration from solutions and wet fiber spinning. *Biomacromolecules* 2005, *6*, 1722-1731.
- 506 [46] Nam, J.; Park, Y.H. Morphology of regenerated silk fibroin: Effects of freezing temperature,
- 507 alcohol addition, and molecular weight. J. Appl. Polym. Sci. 2001, 81, 3008-3021.
- 508 [47] Cestari, M.; Muller, V.; Rodrigues, J.H.D.; Nakamura, C. V.; Rubira, A. F.; Muniz, E. C.
 509 Preparing Silk Fibroin Nanofibers through Electrospinning: Further Heparin Immobilization toward
 510 Hemocompatibility Improvement. *Biomacromolecules* 2014, *15*, 1762-1767.
- 511 [48] Nogueira, G.M.; Rodas, A.C.D.; Leite, C.A.P.; Giles, C.; Higa, O.Z.; Polakiewicz, B.; Beppu,
 512 M.M. Preparation and characterization of ethanol-treated silk fibroin dense membranes for
 513 biomaterials application using waste silk fibers as raw material. *Bioresource Technol.* 2010, *101*,
 514 8446-8451.
- [49] Woo, S.L.; Gomez, M.A.; Seguchi, Y.; Endo, C.M.; Akeson, W.H. Measurement of
 mechanical properties of ligament substance from a bone-ligament-bone preparation. *J. Orthop. Res.* 1983, *1*, 22-9.
 - 518 [50] Ayutsede, J.; Gandhi, M.; Sukigara, S.; Micklus, M.; Chen, H. E.; Ko, F. Regeneration of
 519 Bombyx mori silk by electrospinning. Part 3: characterization of electrospun nonwoven mat.
 520 *Polymer* 2005, *46*, 1625-1634.

- 521 [51] Shields, K. J.; Beckman, M. J.; Bowlin, G. L.; Wayne, J. S. Mechanical properties and cellular
- 522 proliferation of electrospun collagen type II. *Tissue Eng.* **2004**, *10*, 1510-1517.
- 523 [52] Carrizales, C.; Pelfrey, S.; Rincon, R.; Eubanks, T. M.; Kuang, A.; McClure, M. J.; Bowlin, G.
- 524 L.; Macossay, J. Thermal and mechanical properties of electrospun PMMA, PVC, Nylon 6, and
- 525 Nylon 6,6. *Polym. Advan. Technol.* **2008**, *19*, 124-130.
- [53] Lee, K. H.; Kim, H. Y.; Ryu, Y. J.; Kim, K. W.; Choi, S. W. Mechanical behavior of
 electrospun fiber mats of poly(vinyl chloride)/polyurethane polyblends. *J. Polym. Sci. Pol. Phys.*2003, 41, 1256-1262.
- 529 [54] Tan, E.P.S.; Ng, S.Y.; Lim, C.T. Tensile testing of a single ultrafine polymeric fiber.
 530 *Biomaterials* 2005, *26*, 1453-1456.
- 531 [55] Zhang, Y.Z.; Venugopal, J.; Huang, Z.M.; Lim, C.T.; Ramakrishna, S., Crosslinking of the
 532 electrospun gelatin nanofibers. *Polymer* 2006, *47*, 2911-2917.
- 533 [56] Ojha, S.S.; Stevens, D.R.; Stano, K.; Hoffman, T.; Clarke, L. I.; Gorga, R.E. Characterization
 534 of electrical and mechanical properties for coaxial nanofibers with poly(ethylene oxide) (PEO) core
 535 and multiwalled carbon nanotube/PEO sheath. *Macromolecules* 2008, *41*, 2509-2513.
- 536 [57] Ayutsede, J.; Gandhi, M.; Sukigara, S.; Ye, H.; Hsu, C.M., Gogotsi, Y.; Ko, F. Carbon
 537 nanotube reinforced Bombyx mori silk nanofibers by the electrospinning
 538 process. *Biomacromolecules* 2006, *7*, 208-214.
 - 539 [58] Guzman-Puyol, S.; Ceseracciu, L.; Heredia-Guerrero, J.A.; Anyfantis, G.C.; Cingolani, R.;
 - 540 Athanassiou, A.; Bayer, I.S. (2015). Effect of trifluoroacetic acid on the properties of polyvinyl
 - alcohol and polyvinyl alcohol–cellulose composites. *Chem. Eng. J.* **2015**, *277*, 242-251.
 - [59] Rosso, F.; Giordano, A.; Barbarisi, M.; Barbarisi, A. From cell-ECM interactions to tissue
 engineering. J. Cell. Physiol. 2004, 199, 174-180.

Table legend

Table 1. Mechanical properties (apparent elastic modulus, ultimate tensile strength, elongation at yield and elongation at maximum load) of nanofibers. Data are expressed as mean \pm s.d. (n \geq 5). For parsley:fibroin sample, the two values of elastic modulus corresponding to the two different mechanical behaviors are indicated.

Figure legends

Figure 1. Schematic of the main components of (A) Bombyx mori cocoon and (B) parsley stem
residues, and relative organization at different scales.

Figure 2. SEM images of the electrospun nanofibers: (A) fibroin, (B) MCC:fibroin and (C)
parsley:fibroin. Histograms showing the width distribution of the nanofibers: (D) fibroin, (E)
MCC:fibroin and (F) parsley:fibroin.

Figure 3. (A) ATR-FTIR spectra of the electrospun nanofibers. (B) Contribution to amide (%) from
deconvolution of the amide I region of the ATR-FTIR spectra. (C) XRD patterns of the electrospun
nanofibers. (D) TGA thermograms and derivative thermogravimetric curves of the electrospun
nanofibers.

Figure 4. (A) Stress-strain curves of the electrospun nanofibers. Inset: photograph of the nanofibers just after the electrospinning process. (B) Mechanical parameters for the electrospun nanofibers calculated from the stress-strain curves. For parsley:fibroin sample, the two values of elastic modulus corresponding to the two different mechanical behaviors are indicated. (C) Elongation versus elastic modulus data and (D) ultimate tensile strength versus elastic modulus data where other nanofibers prepared using electrospinning are showed.

Figure 5. AFM mappings of the electrospun nanofibers showing the indentation stiffness of fibroin,
MCC:fibroin and parsley:fibroin nanofibers. The map homogeneity indicates good mixing of the
components.

Figure 6. Viability of fibroblast cells (MTT assay) on the different types of nanofibers. Mean \pm standard deviation (n = 3) (A). Fluorescence micrographs of fibroblast cells cultured on (B, E) fibroin, (D, F) MCC: fibroin and (D, G) parsley: fibroin nanofibers.

ACS Biomaterials Science & Engineering

Figure S1. Deconvolution of amide I absorption for fibroin, MCC:fibroin, and parsley:fibroin nanofibers. Black line represents the real absorption, while color lines represent the different contributions. They are marked as random coil (R), beta-sheets (B), alpha-helices (A), turns (T), and side chains (SC).

Figure S2. Detail of the electrospun parsley:fibroin nanofibers showing the crimped waveform
organization of the fibers.

Table of Contents Graphic.





Figure 1. Schematic of the main components of (A) Bombyx mori cocoon and (B) parsley stem residues, and relative organization at different scales. 159x154mm (300 x 300 DPI)



Figure 2. SEM images of the electrospun nanofibers: (A) fibroin, (B) MCC:fibroin and (C) parsley:fibroin. Histograms showing the width distribution of the nanofibers: (D) fibroin, (E) MCC:fibroin and (F) parsley:fibroin. 167x191mm (300 x 300 DPI)





Figure 3. (A) ATR-FTIR spectra of the electrospun nanofibers. (B) Contribution to amide (%) from deconvolution of the amide I region of the ATR-FTIR spectra. (C) XRD patterns of the electrospun nanofibers. (D) TGA thermograms and derivative thermogravimetric curves of the electrospun nanofibers. 159x82mm (300 x 300 DPI)



Figure 4. (A) Stress-strain curves of the electrospun nanofibers. Inset: photograph of the nanofibers just after the electrospinning process. (B) Mechanical parameters for the electrospun nanofibers calculated from the stress-strain curves. For parsley:fibroin sample, the two values of elastic modulus corresponding to the

two different mechanical behaviors are indicated. (C) Elongation versus elastic modulus data and (D) ultimate tensile strength versus elastic modulus data where other nanofibers prepared using electrospinning are showed.

228x236mm (300 x 300 DPI)



Figure 5. AFM mappings of the electrospun nanofibers showing the indentation stiffness of fibroin, MCC:fibroin and parsley:fibroin nanofibers. The map homogeneity indicates good mixing of the components. 160x229mm (300 x 300 DPI)







Figure 6. Viability of fibroblast cells (MTT assay) on the different types of nanofibers. Mean ± standard deviation (n = 3) (A). Fluorescence micrographs of fibroblast cells cultured on (B, E) fibroin, (D, F) MCC:fibroin and (D, G) parsley:fibroin nanofibers. 199x85mm (300 x 300 DPI)