



Predicting the therapeutic efficacy of MSC in bone tissue engineering using the molecular marker *CADM1*

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ABSTRACT

Mesenchymal stromal cells (hMSCs) are advancing into the clinic but the therapeutic efficacy of hMSCs faces the problem of donor variability. In bone tissue engineering, no reliable markers have been identified which are able to predict the bone-forming capacity of hMSCs prior to implantation. To this end, we isolated hMSCs from 62 donors and characterized systematically their *in vitro* lineage differentiation capacity, gene expression signature and *in vivo* capacity for ectopic bone formation. Our data confirms the large variability of *in vitro* differentiation capacity which did not correlate with *in vivo* ectopic bone formation. Using DNA microarray analysis of early passage hMSCs we identified a diagnostic bone-forming classifier. In fact, a single gene, *CADM1*, strongly correlated with the bone-forming capacity of hMSCs and could be used as a reliable *in vitro* diagnostic marker. Furthermore, data mining of genes expressed correlating with *in vivo* bone formation represented involvement in neurogenic processes and Wnt signaling. We will apply our data set to predict therapeutic efficacy of hMSCs and to gain novel insight in the process of bone regeneration. Our bio-informatics driven approach may be used in other fields of cell therapy to establish diagnostic markers for clinical efficacy.

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1. Introduction

Many human diseases are caused by failure of tissue function, with well-known examples such as diabetes, damage inflicted by myocardial infarcts and degeneration of the hip joint. The disciplines of tissue engineering and cell therapy aim at restoring worn-out or diseased tissues for which the patient's own body represents a source of autologous cells [1]. For instance, a much used source of autologous cells in the field of bone tissue engineering is human multipotent mesenchymal stromal cells (hMSCs), also referred to as mesenchymal stem cells [2]. Because hMSCs can be easily isolated from bone marrow aspirates and expanded *in vitro*, they are used for various cell-based therapeutic applications [3]. hMSCs are multipotent cells which are able to differentiate, depending on the

stimulus, into several lineages including the osteogenic, chondrogenic and adipogenic lineage *in vitro* [4]. Osteogenic differentiation of hMSCs is characterized by expression of alkaline phosphatase (ALP) and the formation of a mineralized extracellular matrix (ECM) containing hydroxyapatite. Molecules such as dexamethasone (dex), 3'-5'-cyclic adenosine monophosphate (cAMP), 1,25-dihydroxyvitaminD (vitD3) and bone morphogenetic protein 2 (BMP-2) are used to drive osteogenic differentiation of hMSCs *in vitro* [5–7]. For bone tissue engineering, we and others have demonstrated ectopic bone formation by seeding hMSCs onto porous calcium phosphate scaffolds and subsequent subcutaneous implantation into immune-deficient mice [8,9]. Although proof of principle exists for bone tissue engineering in animal models [10], clinical application is hampered by large donor variation in the ability of hMSCs to deposit bone tissue *in vivo* [11,12]. Unfortunately, bone tissue engineering efficacy is not correlated to known clinical or molecular labels. This is partly due to the fact that the field of hMSC biology lacks an elaborate classification system of CD markers to define stem cells, progenitor

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cells and differentiated cells as it is known for the hematopoietic stem cell system. Cell surface markers such as Stro-1 and the nerve growth factor receptor have been used to prospectively isolate clonogenic hMSCs from a crude bone marrow aspirate [13,14], but the resultant population of cells is still heterogenic in its biological performance. CD146 defines an hMSC subpopulation with the ability to organize a hematopoietic niche *in vivo* but its expression on hMSCs does not correlate to bone formation per se [15]. Therefore, it would be beneficial to define diagnostic markers in culture expanded hMSCs which can predict their *in vivo* performance. The markers could be used to select patients eligible for clinical trials but also provide biological tools to interfere with the osteogenic potential of hMSCs.

The use of diagnostic markers for tissue engineering outcome is successfully used in the field of cartilage regeneration, where Dell'Accio et al. identified a set of molecular markers predictive for *in vivo* cartilage formation of adult human articular chondrocytes [16]. The genes were identified based on their known involvement in the chondrogenic process and similarly, we and others have tried to correlate the expression of genes involved in the osteogenic process in hMSCs to their potency to form bone *in vivo*. Although correlations were found between collagen type I and osteoprotegerin [17] or ALP expression [18] and bone formation, the data sets used were too small to firmly establish a link between gene expression and bone formation and no new insight in the process was obtained. To this end, larger data sets are required for which genome-wide gene expression profiling can be applied. Recently, Larsen et al. identified a molecular phenotype for hMSCs with *in vivo* bone-forming capacity by comparing low versus high bone-forming hMSC-TERT cell populations [19]. Also, in the same group Burns et al. described a correlation between *in vivo* bone formation and *in vitro* expression of matrix proteins determined by analysis of the same cell populations in three-dimensional hydroxyapatite-tricalcium phosphate osteospheroid cultures [20]. However, in both cases donor-to-donor variation is not taken into account since both cell populations originate from the same donor, and thus the molecular signature of bone-forming hMSCs remains incomplete.

We have previously reported on a microarray based approach to distinguish metastasizing from non-metastasizing breast tumors starting from RNA isolated from a breast tumor biopsy [21]. In this study, we have used a similar strategy to find *in vitro* diagnostic markers which are able to predict the *in vivo* bone-forming capacity of hMSCs. We developed a bank of hMSCs from 62 different donors, performed various *in vitro* differentiation assays and analyzed the *in vivo* bone formation for each donor. In addition, we determined the gene expression profile of the hMSCs from the different donors and correlated it with the *in vivo* bone-forming capacity (outlined in Fig. 1). In this manuscript, we present a molecular signature of bone-forming hMSCs.

2. Materials and methods

2.1. Isolation and culture of hMSCs

Bone marrow aspirates (5–20 mL) were obtained from donors with written informed consent, and hMSCs were isolated and proliferated as described previously [22]. Briefly, aspirates were resuspended using a 20-gauge needle, plated at a density of 500,000 cells/cm² and cultured in hMSC proliferation medium containing α -MEM (Gibco), 10% heat-inactivated fetal bovine serum (Biowhittaker), 0.2 mM ascorbic acid (Sigma), 2 mM L-glutamine (Gibco), 100 U/mL penicillin with 100 mg/mL streptomycin (Gibco) and 1 ng/mL basic fibroblast growth factor (Instruchemie, Delfzijl, The Netherlands). The serum batch was selected based on proliferation rate and osteogenic differentiation potential. Cells were grown in a humid atmosphere with 5% CO₂. After plating of the bone marrow aspirate, the cells obtained from the first trypsinization were considered as PD (population doubling) 0. Relative population doublings refers to the number of population doublings that cells had undergone, relative to PD 0. Basic medium was composed of proliferation medium without basic fibroblast growth factor, osteogenic medium was composed of basic

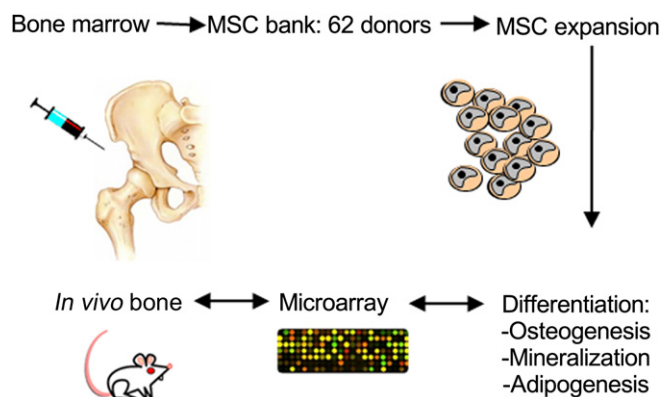


Fig. 1. Study outline. Bone marrow aspirates were obtained from 62 donors, hMSCs were isolated and expanded, subsequently the *in vivo* bone formation, microarray expression profile and differentiation capacity of the cells were determined.

medium supplemented with 10^{-8} M dex (Sigma) and mineralization medium was composed of basic medium supplemented with 10^{-8} M dex and 0.01 M β -glycerophosphate (Sigma). After expansion, cells of the same batch were split into the different media for differentiation assays.

2.2. *In vivo* bone formation

To evaluate the bone-forming capacity of hMSCs, cells were seeded onto porous biphasic calcium phosphate (BCP) ceramic granules of approximately 2–3 mm, prepared and sintered at 1150 °C as described previously [23]. In total, 200,000 cells per three particles were seeded, in osteogenic medium. This seeding density is on the lower hand to avoid an outcome of 100% bone-forming donors. After one week of culturing, tissue-engineered constructs were implanted subcutaneously in immune-deficient mice (Hsd-cbp:NMRI-nu, Harlan, $n = 6$ for each donor). The mice were anesthetized by intramuscular injection of 0.05 mL of 0.5 mg/mL of anesthetic (1.75 mL of 100 μ g/mL ketamine, 1.5 mL of 20 mg/mL xylazine and 0.5 mL of 0.5 mg/mL atropine). Four subcutaneous pockets were made dorsally and each pocket was implanted with three particles. Animals were housed at the Central Laboratory Animal Institute (Utrecht University, Utrecht, The Netherlands), and experiments were approved by the local animal care and use committee. After six weeks, the mice were sacrificed using CO₂ and samples were explanted, fixed in 1.5% glutaraldehyde (Merck) in 0.14 M cacodylic acid (Fluka) buffer (pH 7.3), dehydrated and embedded in methyl methacrylate (LTI) for sectioning. Sections were processed on a histological diamond saw (Leica SP1600). Sections were etched with an HCl/ethanol mixture and sequentially stained to visualize bone, with 1% methylene blue (Sigma) and 0.03% basic fuchsin (Sigma), which stained cells blue and bone pink. Histomorphometry was performed by making low-magnification images from three sections per sample, with a standard selection procedure for each donor. In short, one section in the middle of the scaffold was chosen and the other two sections (left and right side) imaged had the same spacing from the middle section. Scaffold and bone were pseudo colored, and image analysis was performed with KS400 software (Zeiss Vision). A custom-made program (University of Utrecht) was used to measure percentage of bone area compared to scaffold area.

2.3. Mineralization

To determine the mineralization capacity and calcium deposition, hMSCs were seeded in T25 flasks at 5000 cells/cm². Cells were cultured in mineralization medium for three weeks, in triplicate. The total calcium deposition was analyzed by using a Calcium Assay Kit (Quantichrom, BioAssay Systems) according to manufacturer's protocol. Briefly, 0.5 N HCl was used to release calcium and the calcium content was measured at 620 nm and expressed as mg/dl.

2.4. Adipogenesis

Adipogenic differentiation capacity of hMSCs was determined as described previously [24]. In short, after three weeks of culture in adipogenic medium, lipid formation was visualized by staining with Oil red O and staining was quantified by extraction of color and measuring absorbance at 540 nm.

2.5. Chondrogenesis

Cells were grown in pellet culture for 21 days with 250,000 cells/pellet in serum-free chondrogenic medium containing TGF β 3 [25]. Chondrogenic medium was supplemented with 250 ng/mL human BMP6 (Biovision) [26]. Pellets were fixed and stained with Alcian Blue (Sigma).

2.6. Flow cytometry

To analyze ALP expression and expression of CD markers, we used flow cytometry as described previously [24]. For measuring ALP expression, a 1:50 dilution of primary antibody was used (anti-ALP, B4-78, Developmental Studies Hybridoma Bank, University of Iowa) and a 1:100 dilution of secondary antibody (goat-anti-mouse IgG PE, R&D Systems). For cell surface markers, the same procedure was performed using antibodies for CD105, CD11b, CD19, CD45, HLA-DR, CD90 (R&D Systems), CD73 and CD34 (AbCam).

2.7. Western blotting

hMSCs were grown in proliferation medium and hSCLC cells (GLC4, kindly provided by the Department of Medical Oncology, University Medical Center Groningen) were grown in RPMI1640 (Gibco) supplemented with 10% heat-inactivated fetal bovine serum (Biowhittaker) and 100 U/mL penicillin with 100 mg/mL streptomycin (Gibco). Total protein was isolated and quantified using the BCA protein assay kit (Pierce). Cell lysates were separated using sodium dodecyl sulfate polyacrylamide gel electrophoresis and transferred to an Immobilon-P membrane. The membrane was blocked in Tris-buffered saline with 5% milk for 1 h and probed with 0.1 µg/mL polyclonal anti-CADM1 (Santa Cruz, sc-33198), overnight at 4 °C. Next, the membrane was incubated with horseradish peroxidase conjugated goat anti-rabbit IgG (Dako) as the secondary antibody for 1 h at RT. Protein detection was performed by luminescence, using a Kodak image station 4000 MM after incubating the membranes with Supersignal chemiluminescent detection (Pierce) for 2 min.

2.8. Immunofluorescence

hMSCs were seeded and when reaching 60% confluence fixed with 10% formalin for 20 min. After blocking with 1% bovine serum albumin they were probed with 50 times diluted polyclonal anti-CADM1 (Santa Cruz, sc-33198) for 1 h at RT. Next, cells were incubated with Alexafluor488 conjugated goat-anti-rabbit IgG (Invitrogen). As a counterstain we used Alexafluor568 conjugated Phalloidin (Invitrogen) and DAPI (Sigma). Cells were imaged using BD Pathway 435 Bioimager (BD Biosciences).

2.9. Microarray analysis and quantitative polymerase chain reaction

To analyze the gene expression profile of hMSCs, cells were seeded at 1000 cells/cm² and upon reaching near confluence RNA was isolated using an RNeasy mini kit (Qiagen) and DNase treated on column with 10U RNase free DNase I (Gibco) at 37 °C for 30 min. DNase was inactivated at 72 °C for 15 min. The quality and quantity of RNA was analyzed by gel electrophoresis and spectrophotometrically. For qPCR, we performed cDNA synthesis using the iScript cDNA synthesis kit (Bio-rad) and qPCR was carried out using iQ SYBR Green Supermix (Bio-rad). Primer (Sigma) sequences are depicted in Table S2, as a reference gene we used *GAPDH* or *B2M* (see figure legends). For *GPM6B* we used primers which were commercially available (SA Biosciences, annealing temperature 55 °C). For all other genes we used 3 mM MgCl₂ and an annealing temperature of 60 °C. To test significance we use a paired student's *t*-test. For microarray analysis, the RNA was hybridized to the Human Genome U133A 2.0 Array (Affymetrix) and scanned with a GeneChip G3000 scanner (Affymetrix). The microarray experiments were performed in three batches. To normalize the measurements, we used a normalization method which removes hybridization, amplification and array location based technical effects. To determine the most significant genes with respect to a label-set, we determined a (two-sided) *p*-value for each gene using a permutation test. As test statistic we used the significant analysis of microarrays [27] test statistic [28] for class labels and the F-test for continuous labels. In total, for each label-set, we performed 10,000 permutations. Genes were sorted on their estimated *p*-value. For further analysis, we also calculated gene set enrichments using gene sets from the database of molecular signatures (MsigDB) [29]. In addition to this, we trained a classifier for the binary bone label (bone or no bone), predicting if bone formation would occur for a certain donor or not. We applied a Nearest-Mean classifier (available as part of PRTTools, [30]), and performance was estimated using leave-one-out cross-validation. The probesets to be used as features were selected by taking those with the highest SAM test statistic value on the training set. To determine the optimal number of probesets an inner leave-one-out cross-validation loop was performed. An area under curve (AUC) score of the Receiver Operating Characteristic (ROC), a widely used standard for describing and comparing the accuracy of diagnostic tests, was constructed by combining results for the different validation sets using the classifier class probability (determined using maximum likelihood posterior probabilities [30]). ROC represents the tradeoff between the false negative and false positive rates for every possible cut-off. AUC is a measure of the probability that a classifier based on this label would rank a randomly chosen positive donor higher than a randomly chosen negative donor, where AUC = 1 is a perfect ranking classifier and AUC = 0.5 depicts complete randomness.

2.10. Micro-CT scanning

To evaluate differences in bone architecture of *CADM1* knockout and wild type mice, femora of each were selected for micro-CT scanning. Micro-CT scans were

acquired using the SkyScan 1076 scanner (Kontich, Belgium) with a 9 µm-resolution protocol (50 kV energy, 200 µA current, 1.0 mm Al filter) and reconstructed using NRecon software 1.6 (SkyScan, Kontich, Belgium). With Dataviewer 1.4, a segment of the distal metaphysis (10 mm) was selected as region of interest. To distinguish calcified tissue from non-calcified tissue and noise, the reconstructed grayscale images were segmented by an automated algorithm using local thresholds [31], resulting in a 3D data set consisting of stacked black/white cross-sections. Cortical and trabecular bone were subsequently automatically separated using in-house software. Trabecular architecture of the metaphysis was characterized by determining the trabecular bone volume fraction (BV/TV), which is the ratio of trabecular bone volume over endocortical tissue volume. Connectivity density, structural model index, trabecular thickness and trabecular separation were also calculated.

2.11. *CADM1* knockout mice

The femora and skulls from homozygous *CADM1* knockout mice were obtained from RIKEN BioResource Centre (B6.129S6-Cadm1<tm1Momo>, RBRC04063; Japan). The knockout mice were developed by Takashi Momoi as described previously [32] and deposited at the BioResource Centre. Femora were explanted from both knockout and wild type mice of two distinct ages. One group consisted of 8-week old mice (3 knockout and 2 wild type) and the other group consisted of 11-week old mice (4 knockout and 3 wild type). The femora and skull of the mice (C57BL/6j) were explanted and fixed for 24 h in paraformaldehyde and subsequently transferred to PBS. External differences between the knockout samples and wild type were measured. For the skulls, different diameters were compared between the samples. Detailed information about micro-CT scanning can be found in supplementary text S1.

3. Results

3.1. Large inter-donor variability in biological characteristics of hMSCs

To find a predictive marker for bone formation by hMSCs *in vivo* we aspirated bone marrow from either the acetabulum or the iliac crest of 62 donors undergoing orthopedic surgery, 48 of which were female and 15 were male. The age of the donors varied from 17 to 84 years with an average of 56 years. Aspirates were put into culture and the identity of the proliferating hMSCs was confirmed according to the set of standards proposed by the Mesenchymal and Tissue Stem Cell Committee of the International Society for Cellular Therapy [33]. The cells were adherent to plastic (Fig. S1A) and more than 94% expressed CD73 and CD90, 60% expressed CD105, and less than 2% expressed CD45, CD34, CD11b, CD19 and HLA-DR, as measured by flow cytometry in hMSCs isolated from three donors (Fig. S1C). Moreover, we were able to differentiate the cells into the osteogenic, adipogenic and chondrogenic lineage under standard *in vitro* differentiation conditions, as demonstrated by histological staining (Fig. S1B).

To show that donor variability in the bone-forming capacity exists within this set of hMSCs, we used the ectopic bone formation model in immune-deficient mice [6,15,34–36] to quantify ectopic bone formation *in vivo*. To this end, hMSCs of all donors were seeded onto porous calcium phosphate ceramic scaffolds and cultured for one week in osteogenic medium, prior to implantation (*n* = 6). After six weeks, scaffolds were explanted and bone formation was quantified (Fig. S2). Out of 62 donors, 35 did show bone formation ranging from 0.01 to 4.6% of bone area compared to scaffold area demonstrating a large inter-donor variability (Fig. 2E).

To further investigate donor variability, we characterized the hMSCs for a number of cellular parameters, such as proliferation and *in vitro* differentiation. Indeed, we observed large differences in the rate of hMSC proliferation (Fig. 2A) and osteogenic differentiation, indicated by the potency of dexamethasone (dex) to enhance the expression of the early osteogenic marker ALP. As reported by us previously, both basic and dex-induced expression of ALP showed large donor variation [11]. ALP expression in the control group ranged from 0.2 to 39% of ALP positive cells and in the dex-induced group from 0.3 to 47%, with an average of 12% (Fig. 2B, Table S1). Likewise, large donor variation was observed in the

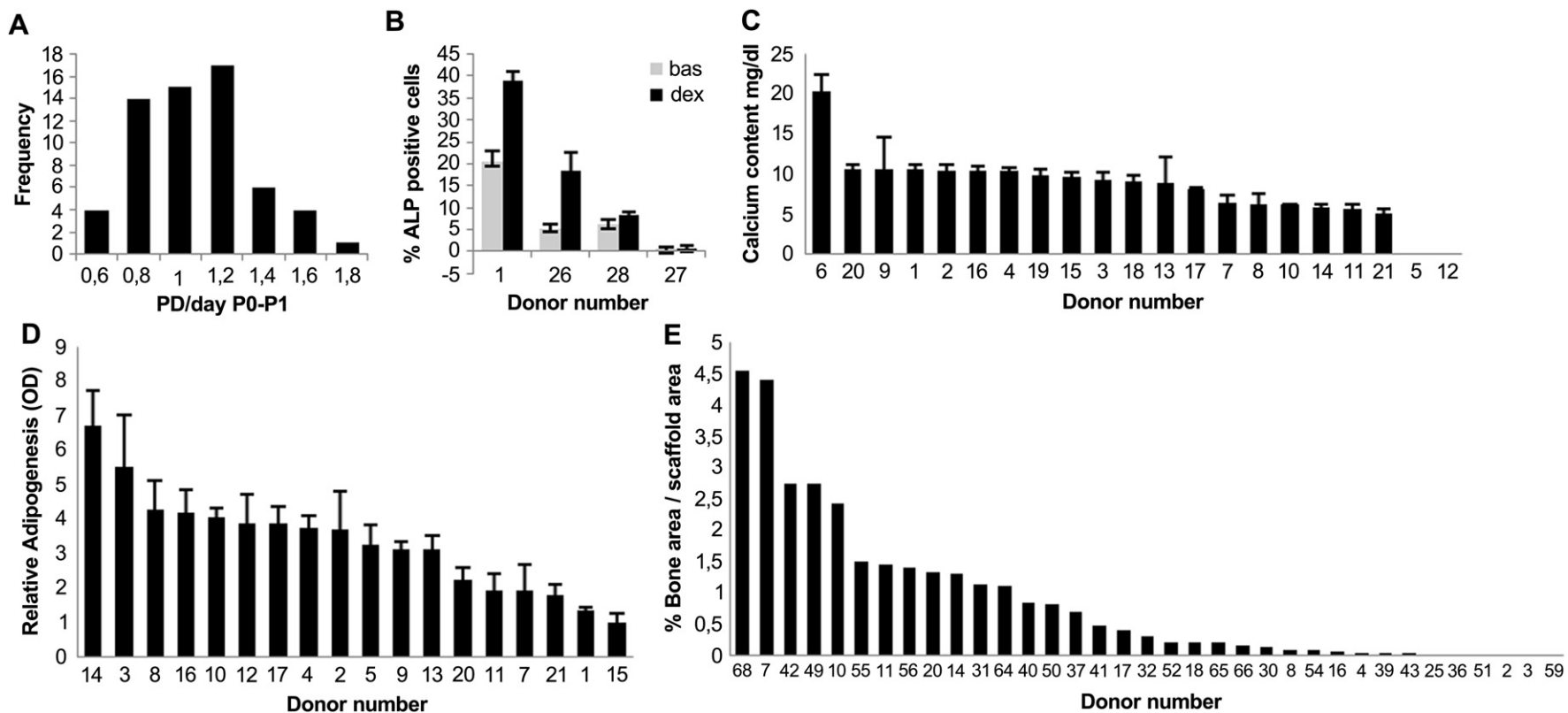


Fig. 2. Characterization of hMSCs. A) Proliferation; hMSCs were cultured and counted when reaching 70–80% confluence. Frequency of population doublings (PD) per day was calculated, passage 0–1, for 61 donors in total. B) ALP expression; hMSCs were cultured in basic (bas) or osteogenic (dex) medium during seven days. The percentage of ALP positive cells was determined using flow cytometry. Error bars represent the standard deviation. Here we show an example for four donors, in Table S1 all values are depicted. C) Mineralization; hMSCs were seeded at 5000/cm² and cultured in mineralization medium for three weeks. HCl was used to release calcium and calcium deposition was measured and expressed as mg/dl sample. Error bars represent the standard deviation. D) Adipogenesis; hMSCs were cultured in adipogenic medium for three weeks. Adipogenic differentiation was visualized by staining with Oil red O; the color was extracted and measured spectrophotometrically. Error bars represent the standard deviation. E) *In vivo* bone formation of hMSCs; hMSCs were cultured on BCP particles (200,000 cells/3 particles) in osteogenic medium for seven days and implanted subcutaneously in nude mice for six weeks. Out of 62 donors, 35 showed bone formation. Histomorphometric analysis demonstrated the large variation between donors.

mineralization capacity of hMSCs, which is a late marker for *in vitro* osteogenesis. The ability of the cells to deposit a mineralized matrix ranged from 0 to 20.3 mg/dl of calcium, with an average of 8.3 (Fig. 2C). Similarly, the adipogenic differentiation capacity of hMSCs was determined by quantification of lipid formation after 3 weeks of culture in adipogenic medium. In effect, the optical density (OD) ranged from 1 to 6.7 with an average of 3.3 in 18 different donors (Fig. 2D). In conclusion, the biological performance of hMSCs varied strongly between donors, both *in vivo* and *in vitro*.

3.2. Correlation between cell biological data labels, donor features and bone formation

Differential bone apposition of hMSCs may be correlated to some of the cellular or physiological parameters associated with the hMSCs, as described above, or to the donors from which they were isolated, e.g. gender, age or site of aspiration. Therefore, all available parameters and measured variables were quantitatively correlated to bone formation *in vivo*. As an example, ALP activity is commonly used to describe osteogenic differentiation *in vitro*. It also has been

shown previously that hMSCs undergo rapid senescence during *in vitro* culture and lose their ability to differentiate [11].

Consequently, we were interested in assessing the correlation of these parameters and the *in vivo* bone-forming capacity of hMSCs. However, no significant correlation between both ALP expression or proliferation rate of hMSCs and bone formation could be detected (Fig. 3A and B). To further investigate the possibility to use these 2 parameters as a marker able to classify bone-forming versus non bone-forming donors, we produced a Receiver Operating Characteristic (ROC) curve (Fig. 3C). These data indicate that neither ALP activity nor proliferation rate is able to predict the bone-forming capacity of hMSCs *in vivo*. Next, we investigated whether other cell biological features such as number of mononuclear cells per mL of bone marrow, amount of mineralization or adipogenic differentiation, or donor features such as surgery type, site of aspiration, gender or age correlated with the bone-forming capacity. To this end, ROC curves for all these parameters were generated and the areas under curve (AUCs) with corresponding *p*-values were calculated for all labels (Fig. S3A). As can be observed in Fig S3A, significance was not found for any single parameter after

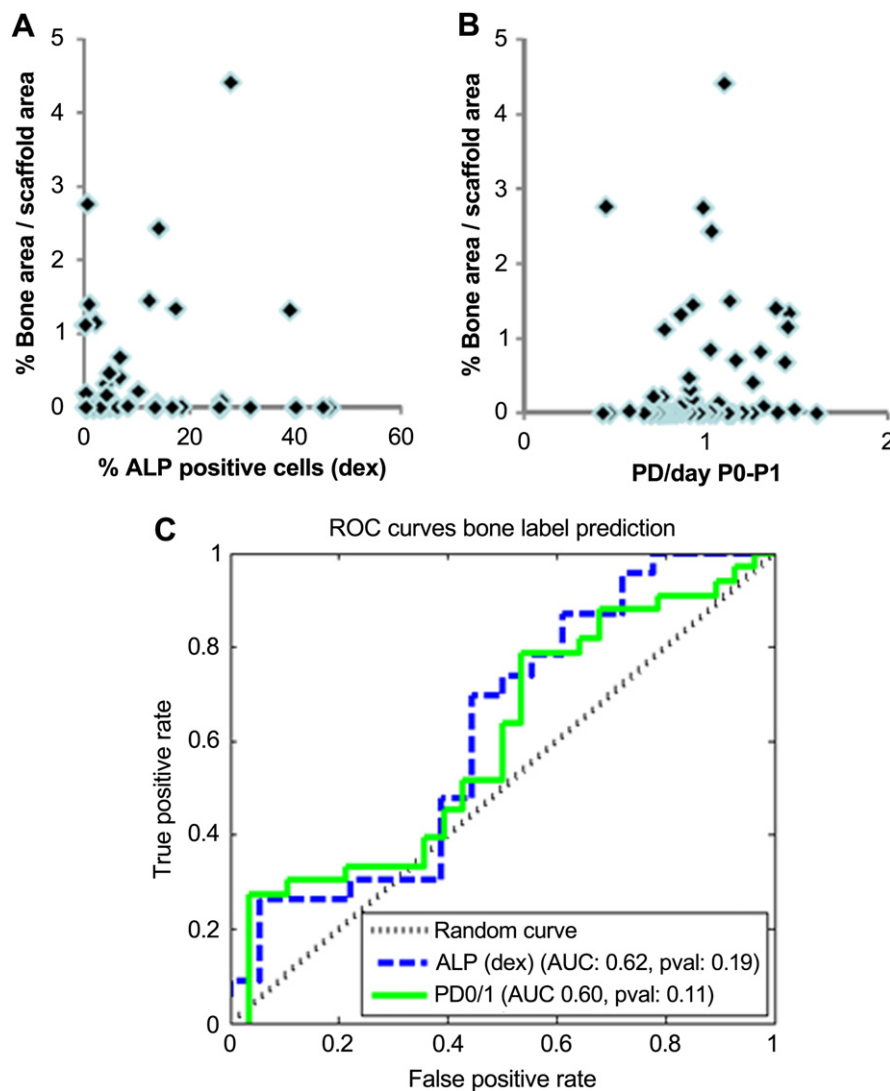


Fig. 3. Correlation between cell biological data labels, donor features and *in vivo* bone formation. A correlation curve was created by plotting the different parameters against the *in vivo* bone formation. An example is shown of percentage of ALP positive cells (dex) (A) or proliferation doublings per day (B). No correlation was found with all data labels. C) Receiver Operating Characteristic (ROC) curves to represent the tradeoff between the false negative and false positive rates for every possible cut-off. The AUC (area under curve) was calculated for all labels, which is a measure of the probability that a classifier based on this label would rank a randomly chosen positive donor higher than a randomly chosen negative donor. The data indicate that neither ALP activity nor proliferation rate correlate with bone-forming capacity *in vivo*.

multiple testing correction, neither when the presence or absence of bone was used as a cut-off, nor when the threshold was based on percentage of bone apposition where the amount of bone formed was taken into account. Next, we tried to build a classifier combining both the clinical and biological data, since multiple labels combined may provide a higher predictive value (see Materials and Methods section). The best AUC obtained among all labels for imputation based strategies (i.e. classifier on all donors) was 0.59, which is slightly above random.

3.3. A single gene bone classifier based on whole genome gene expression profiling

Since no cellular or physiological markers could be identified for *in vivo* bone formation by hMSCs, we determined their genome-wide gene expression profile to find genes which' expression could be correlated with *in vivo* bone formation. Therefore, RNA was isolated from undifferentiated hMSCs during the expansion phase in passage two and hybridized to Human Genome U133A 2.0 Arrays (Affymetrix). A diagnostic classifier was built based on the gene expression profiles of the different hMSCs and evaluated on its ability to predict bone-forming capacity. For this purpose, we trained a nearest-mean classifier, using the SAM test statistic to select the genes (see Materials and Methods section). Since we aimed at identifying diagnostic markers able to distinguish bone-forming from non bone-forming donors, only genes displaying a relatively large difference between different hMSCs (standard deviation between arrays > 0.4) were considered. Hence, a list of genes correlating with the *in vivo* bone formation of hMSCs was selected from the remaining 1653 probesets (out of 22,277 genes). Interestingly, in the top 50 of probes (Table 1), 15 genes have been implicated in bone formation before such as *IGF1* [37], *WISP1* [38] and *DKK1* [39] and 11 genes are reported to be implicated in neural adhesion and neuronal functioning such as *CADM1* [40], the neurotransmitter receptor *GABBR2* [41] and carboxypeptidase E [42]. To calculate the predictive value of the probes, ROC curves were created (Fig. 4A), giving the result for different threshold values of the classifier. The best performing classifier showed an AUC score of 0.76, compared to 0.59 for the best clinical classifier. Interestingly, this performance could already be reached using only one probeset (Fig. 4B). We found that in all folds of the cross-validation, the top probe set was the same, which detects the *CADM1* gene. The performance of all *CADM1* probes on the microarray was assessed by calculating the AUC score for each probe (Fig. S4A). Most of the probes showed similar AUC scores, though some of them showed lower values, these were not shown to correlate with possible splice-variants. The *p*-values were

calculated (Fig. S4B), showing near significance between the different probes.

Since some factors related to bone formation change their expression before and after the menopause in female donor samples we investigated if this was the case for *CADM1*. As no information is available on the onset of the menopause for the donors in this study, we selected all female donors before age 40 as pre-menopause, and female donors after age 61 as post-menopause [43]. This resulted in a set of respectively 10 and 20 donors.

We did not find any significant change in *CADM1* expression between pre-menopause and post-menopause females (ranksum-test *p*-value 0.74). Next, we tested if the strength of the relation of *CADM1* with bone-forming was different for pre-menopause and post-menopause female donors. While we found a substantial difference in AUCs (0.71 versus 0.87), a permutation test did not show this difference to be significant (*p*-value 0.31). In short, while there might be menopause effects, we could not proof this conclusively.

To validate the results obtained by microarray analysis, gene expression data of a number of genes in the top of the gene list was reproduced using quantitative polymerase chain reaction and with these data, ROC curves were created (Fig. 4C). Some of the genes validated by qPCR did show a good correlation with AUCs in the range of the *CADM1* microarray data (which was 0.76) such as the Wnt target gene *WISP1*, with a positive correlation to bone formation (AUC 0.73), *CPE* (AUC 0.72) or the Wnt antagonist *DKK1* with a negative correlation to bone formation (AUC 0.63). Moreover, the positive correlation between bone formation and *CADM1* expression was confirmed by qPCR with an AUC score of 0.84.

To confirm that the *CADM1* protein is expressed in hMSCs we performed immunostaining and Western blotting (Fig. S5A). In human small cell lung cancer cells (hSCLC), known to express the *CADM1* protein, we observed one band at the expected size of 60 kD. In hMSCs, however, three bands of 60, 75 and 250 kD were observed. The 250 kD and 75 kD bands are most likely post-translationally modified proteins since *CADM1* is known to be prone to polysialylation and glycosylation [44]. Immunostaining of *CADM1* in hMSCs resulted in a mainly perinuclear appearance of the protein (Fig. S5B).

3.4. Decreased expression of predictive markers upon *in vitro* expansion

hMSCs lose their multipotency upon *in vitro* expansion [11,45] and specific hMSC markers, such as STRO-1 [46] and NGFR, are known to show concomitant decrease in expression. Therefore, we were interested to analyze the expression of a selection of marker genes from our list, identified to correlate to bone formation, during expansion in six different donors (Fig. 5). The expression of *CADM1* (Fig. 5A) and *CPE* (Fig. 5C) decreased after expansion and interestingly, expression of *DKK1*, which we found to be negatively correlated with bone formation, did increase (Fig. 5B). Expression of other genes in the top list did not change, such as *WISP1* (Fig. 5D), *GPM6B* (Fig. S6A) and *MYO1D* (Fig. S6B). As a control we confirmed that expression of housekeeping genes β -actin (Fig. S6C) and 18S (Fig. S6D) did not change. In conclusion, expansion of hMSCs had an overall negative effect on expression of marker genes correlating with *in vivo* bone formation.

3.5. No distinct bone phenotype in *CADM1* knockout mice

Although *CADM1* has been associated with a number of biological functions, such as heterotopic cell–cell interaction, this gene has never been related to bone homeostasis. In order to explore this relation, femur bones were explanted from homozygous *CADM1* knockout mice and scanned by micro-CT. Bone mineral density was

Table 1
Genes correlating with *in vivo* bone formation in hMSCs.^a

Neuronal	Osteogenesis	WNT/IGF-signaling	Miscellaneous/unknown	
<i>CADM1</i>	<i>HMG2A2</i>	<i>IGF1</i>	<i>CXCR7</i>	<i>CRISPLD2</i>
<i>GABBR2</i>	<i>S100A4</i>	<i>WISP1</i>	<i>SEPP1</i>	<i>FAM38B</i>
<i>SEMA5A</i>	<i>COL14A1</i>	<i>DKK1</i>	<i>HNMT</i>	<i>TXNIP</i>
<i>GPM6B</i>	<i>PCOLCE2</i>	<i>HOXB7</i>	<i>EVI2A</i>	<i>ECM2</i>
<i>CPE</i>	<i>SOX9</i>	<i>WISP2</i>	<i>OLFML1</i>	<i>PSPH</i>
<i>ADAM19</i>	<i>GPM6B</i>	<i>SOCS2</i>	<i>KCNK2</i>	<i>STAT4</i>
<i>NRN1</i>	<i>GABBR2</i>		<i>PNMAL1</i>	<i>LL22NC03-75B3.6</i>
<i>SHOX2</i>	<i>SHOX2</i>		<i>VCAM1</i>	<i>GALNT6</i>
<i>ENPP2</i>	<i>OXTR</i>		<i>LUM</i>	<i>DCN</i>
<i>OXTR</i>			<i>IGL</i>	<i>IFI44</i>
<i>MYO1D</i>			<i>GOS2</i>	

^a Top 50 of probes correlating with the *in vivo* bone formation of hMSCs. Some genes were present twice or more since multiple probes per gene were analyzed, these genes are only depicted once in this list.

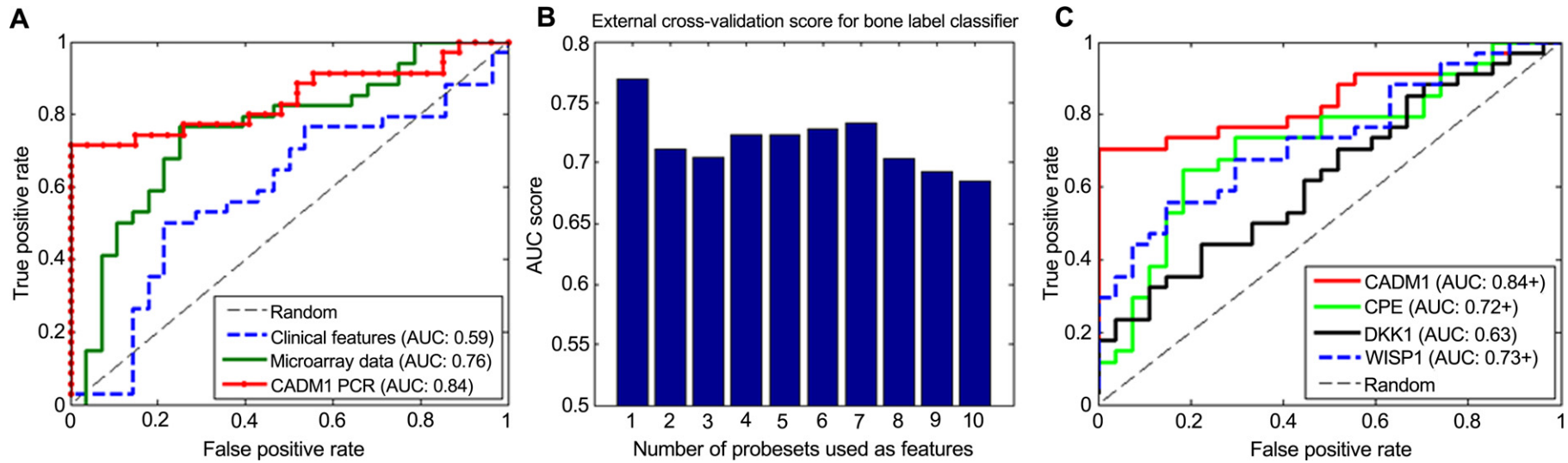


Fig. 4. Classifier performance on the bone labels. Classifier performance on the separation of bone-forming donors from non bone-forming donors. The performance is presented using ROC curves (which represent the tradeoff between false negative and false positive rates for every possible classifier threshold) and the AUC (Area Under ROC curve) score (which represents the probability that the classifier would rank a randomly chosen positive donor higher than a randomly chosen negative donor). A) ROC performance curves of classifiers using either clinical features, microarray probesets or *CADM1* qPCR data (normalized for *GAPDH* expression). ROC curves were obtained by using the posterior probabilities of the validation samples of the leave-one-out cross-validation procedure. Features (probesets) were ranked by using the SAM test statistic within the cross-validation loop. The optimal number of features to select from the top of the ranked list was determined using an inner cross-validation loop. Interestingly, the optimal microarray performance was reached using only one probeset, measuring *CADM1*. No feature selection (and thus cross-validation) was necessary for *CADM1* qPCR. B) AUC score for the microarray data set, using a fixed number of features from the top of the ranked list. The top probeset in every cross-validation fold was *CADM1*. C) qPCR validation of the microarray results (normalized for *GAPDH* expression). Some of the genes were not predictive for bone formation *in vivo*, others did show a good correlation with AUCs in the range of the *CADM1* microarray data.

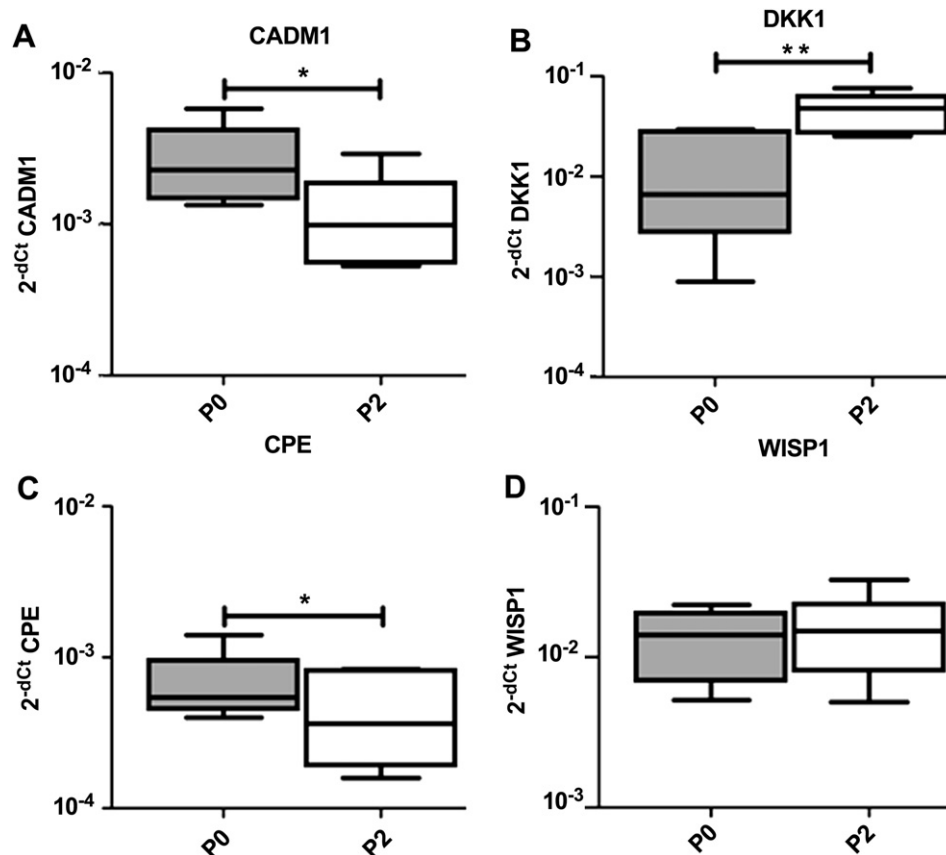


Fig. 5. Expression of predictive markers upon expansion. hMSCs of six different donors were cultured and after passage 0 and 2 RNA was isolated and qPCR was performed (normalized for *B2M* expression) to analyze expression of *CADM1* (A), *DKK1* (B), *CPE* (C) and *WISP1* (D). *CADM1* and *CPE* expression decreased after expansion, and interestingly, *DKK1* expression (which was negatively correlated to bone formation) increased. Expression of *WISP1* did not change. Error bars represent the standard deviation, for significance a paired student's *t*-test was used (* $p < 0.05$, ** $p < 0.01$).

assessed by measuring the bone volume fraction within the endocortical area of the metaphysis region. The bone volume fraction did not differ between the *CADM1* knockout mice and the wild type mice for both 8-week old and 11-week old mice. The other parameters commonly used to distinguish any bone phenotype, such as trabecular separation, trabecular thickness, connectivity density (number of redundant connections between trabecular structures per unit volume), structural model index (prevalence of a particular trabecular shape), also showed no significant changes within the *CADM1* knockout mice (Fig. S7).

4. Discussion

hMSCs have been targeted as potential source for autologous bone tissue engineering almost two decades ago and have been tested in phase 1 clinical trials [47]. Further evaluation is severely hampered by the large donor-to-donor variation in bone apposition. So far, no reliable markers exist that could help sort out “good” from “bad” donors. In our set, we were not able to link bone formation to any of the donor or cellular labels that were analyzed. Using *CADM1* gene expression profiling, we were able to obtain an AUC score of 0.84 for the whole donor set. In practical terms, this means for instance that using *CADM1* expression, we have a tool to include patients into future clinical trials with a high probability of bone apposition. To put this score into perspective, in our experience this is a better performance than what can be obtained with diagnostic marker sets used to distinguish metastatic behavior of breast tumors [48]. It shows that *in vitro* gene expression profiling is an

efficient strategy to find diagnostic markers predicting therapeutic efficacy of stem cell therapy. Using a combination of histology and gene expression profiling we have been able to bridge the gap between the expansion of hMSCs in culture and bone apposition *in vivo*. It is important to realize that this approach can be applied in any strategy where the therapeutic efficacy of a stem cell has to be assessed *in vitro*.

Another potential application of *CADM1* lies in the area of drug discovery. The field of bone tissue engineering puts a lot of effort into optimizing the isolation procedures and culture conditions favoring the bone-forming capacity of hMSCs [6,34]. So far, ectopic bone formation *in vivo* is the golden standard to verify the efficacy of a modification to the bone tissue engineering protocol. With *CADM1* as a predictor of bone formation *in vivo*, we can embark on high throughput screening strategies to identify small molecules that improve the bone-forming capacity of hMSCs. Moreover, we can screen libraries of scaffold materials which favor bone formation by hMSCs. Besides screening, the link between *CADM1* and bone formation may shed light on the bone formation process. *CADM1* protein is involved in a broad, seemingly pleiotropic range of diseases and functions, such as neuronal synapse formation [40], as a tumor suppressor [49], the communication between mast cells and smooth muscle cells [50] and in venous thrombosis [51]. For example, overexpression of *CADM1* in HEK293 cells resulted in synapse formation in co-cultures with neuronal cells [40]. A common signature may be heterotypic cellular interaction, and the concurrent role of hMSCs as trophic mediators in tissue formation is in line with this. With respect to its neuronal role, it is interesting

to note that in the top 20 of genes associated to bone formation, 11 have a neuronal signature. GABBR2 is a neurotransmitter receptor, SEMA5A is a neuronal adhesion molecule, GPM6B is known to play a role in neurotransmitter release and carboxypeptidase E controls neurotransmitter activity.

Beyond *CADM1*, we identified a number of other genes with a correlation to bone formation and some of them have a known role in the osteogenic process. For instance, IGF1 is known to play a role in the mineralization phase of osteogenesis and controlled release of IGF1 in a bone defect is beneficial to the healing process [52]. We have previously identified IGF1 as a cytokine which is strongly upregulated in hMSCs treated with cAMP [6] and associated with enhanced bone formation as well. Oxytocin is an anabolic bone hormone and together with its receptor OXTR, present in our list, regulates bone mass [53]. *SHOX2* has been related to Turner syndrome [54] and as an upstream regulator of *RUNX2* during long-bone development [55]. In fact, the mouse *SHOX2* gene codes for a transcription factor required for the proximal bone formation of the limbs [56]. Moreover, besides its correlation to neuronal functioning, *GPM6B* is reported to be strongly upregulated during osteoblast differentiation and related to alkaline phosphatase activity and matrix mineralization in hMSCs [57]. Similarly, the neurotransmitter receptor GABBR2 is constitutively expressed in murine calvarial osteoblasts and also localized in growth plate and on the membranes of cultured growth plate chondrocytes [58]. GABBR2 was shown to inhibit cAMP formation, ALP activity, and calcium accumulation, and decreases *BMP2*, osteocalcin, and osterix expression. On the other hand, the expression of *ADAM19* was reported in bone-marrow derived mesenchymal stromal cells during chondrogenic differentiation by micropellet culture in the presence of *BMP2* [59].

Another group of interesting genes are those involved in Wnt signaling. In the top 100 of genes associated with bone formation, we can find Wnt target genes *WISP1*, *WISP2* [60], *HOXB7* and *S100A4* [61]. *DKK1*, a negative regulator of Wnt signaling [62] on the other hand is negatively associated to bone formation, which is in line with a positive role of Wnt signaling in bone formation. Ironically, we have previously shown that increased Wnt signaling in hMSCs is negatively correlated to osteogenic differentiation of hMSCs *in vitro* but positively correlated to the rate of hMSC proliferation. In that respect, the relatively low *P*-values correlating proliferation rate and bone formation (Fig. S3B) may be due to high Wnt signaling. We are now investigating the effect of Wnt signaling on bone formation *in vivo*.

We show here that expression of predictive markers decreased upon *in vitro* expansion of hMSCs. Interestingly, *DKK1*, which we found to be negatively correlated to ectopic bone formation, showed an increased expression upon expansion. We tested this in six donors and found again a large donor variation. It is also known that both expression of *Stro-1*, a clonogenic hMSC marker, and *in vivo* bone formation decrease upon expansion [46,63]. For this reason, we are investigating the possibility to directly use the crude bone marrow instead of expanded hMSCs for tissue engineering purposes [64].

Finally, we may isolate the *CADM1* positive fraction, preferably from crude bone marrow, and analyze whether the enrichment in percentage of *CADM1* positive cells has a beneficial effect on bone formation. Furthermore, the analysis of the *CADM1* positive fraction of hMSCs may teach us more about the nature of the bone-forming hMSC. Considering the fact that the ceramics implanted in this study were fully covered by hMSCs, the amount of bone observed was rather low, suggesting that only a small subset of the implanted cells is actually able to enter the osteogenic process. Considering the numerous steps and the long time that separates the moment of gene expression profiling in the expanding hMSCs

and histomorphometric assessment of bone formation in nude mice, it is encouraging to see that *CADM1* expression has a high predictive value. Even though very little to nothing is known about the nature of the bone-forming fraction of hMSCs, we have good hopes that the *CADM1* positive fraction will shed a light on this process.

5. Conclusions

We have correlated the bone-forming capacity of hMSCs in an immune-deficient mouse model to the expression of genes during the expansion phase of hMSC culture. We have identified the *CADM1* gene as a marker which is able to predict bone formation with an AUC of 0.84. Furthermore, we have disclosed a link between the expression of neurogenic genes and bone-forming capacity of hMSCs. Our approach can be applied in any strategy where the therapeutic efficacy of stem cells needs to be assessed. Furthermore, the *CADM1* gene can be used as a tool for screening small molecules or materials on their effect on bone formation.

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Appendix A. Supplementary data

Supplementary data related to this article can be found at <http://dx.doi.org/10.1016/j.biomaterials.2013.03.001>.

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