

# Food Hydrocolloids

## A Millifluidic-assisted ionic gelation technique for encapsulation of probiotics in double-layered polysaccharide structure --Manuscript Draft--

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<b>Abstract:</b>	A unique double-layered probiotic delivery system based on a millifluidic/direct gelation method of encapsulation has been investigated. The effects of variation of alginate concentration (20-30 g/l), flow rates of alginate (0.8-1.2 ml/min), and water/oil (W/O) emulsion (0.5-0.7 ml/min) on emulsion encapsulation efficiency (EE), size, and sphericity (SF) of core-shell millicapsules were examined using a central composite design to optimize a delivery system for the encapsulated <i>Bifidobacterium animalis</i> subsp. <i>lactis</i> and <i>Lactobacillus plantarum</i> . The optimized calcium-alginate millicapsule was spherical ( $0.97 \pm 0.01$ SF), with an average diameter of $4.49 \pm 0.19$ $\mu$ m, and an emulsion encapsulation efficiency of $98.17 \pm 0.5\%$ . Two probiotic strains were encapsulated separately in W/O emulsion as a core of the millicapsule. After coating with chitosan, the encapsulation yield of the bacteria, survival rates under simulated gastrointestinal (GI) conditions, and viability during storage were determined. Survival efficiency values of <i>B. animalis</i> subsp. <i>lactis</i> and <i>L. plantarum</i> after millifluidic encapsulation were found to be 92.33 and 90.81%, respectively. Cell viability of probiotics embedded in the millicapsule after passing through the GI system was improved ( $7.5$ log CFU ml <sup>-1</sup> for both strains). Although the viability of the encapsulated probiotics stored at $-18$ °C for six months significantly decreased ( $p < 0.05$ ), the number of live cells was approximately in accordance with the standard definition of long-term probiotic survival ( $6$ log CFU g <sup>-1</sup> ).
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**Dear Prof. P.A. Williams,**

**Editor-in-Chief of Food Hydrocolloids,**

I wish to submit a new research manuscript entitled ‘‘ **A Millifluidic-assisted ionic gelation technique for encapsulation of probiotics in double-layered polysaccharide structure**’’ for consideration by the journal of Food Hydrocolloids.

This is the first report of using two techniques (Millifluidic and ionic gelation) simultaneously as the ‘‘double-layered strategy platform’’ for encapsulation of probiotic strains.

The ‘‘millifluidic’’ technique could be considered as a ‘‘novel approach’’ for ‘‘encapsulation’’ of ‘‘bioactive compounds’’ and has a promising perspective in the field of food engineering or pharmaceutical science (drug delivery systems). To the best of our knowledge, despite of the advantages of millifluidic technique as an encapsulation process, no study has optimized this method for the encapsulation of probiotic bacteria. Therefore, in this study we aim to optimize the millifluidic technique for the encapsulation of two probiotic bacteria species, *Bifidobacterium animalis* subsp. lactis and *Lactobacillus plantarum*, separately, into optimal W/O emulsion-filled millicapsules and to assess survival rates during storage and the viability of the encapsulated probiotics under simulated GI conditions.

Accordingly, the utility of the millifluidic encapsulation method paves the way for fabrication of a unique carrier for probiotic bacteria. Furthermore, encapsulation of lipophilic compounds in the oil part and hydrophilic compounds in the water part of emulsion loaded in millicapsules can be exploited co-encapsulation in various domains.

This project has successfully been accomplished at Department of Food Nanotechnology, Research Institute of Food Science & Technology (RIFST) and Mashhad University of Medical Science, (IRAN). This novel work has also been internationally extended and professionally supervised by my colleague Dr. Nick Tucker, from University of Lincoln (UK).

I would be most grateful if we could receive the invaluable comments of the reviewers and have a chance to publish our paper in the high prestigious journal of Food Hydrocolloids.

Thank you very much indeed for your consideration of this manuscript.

**Respectfully yours,**

*Behrouz Ghorani*

*12/15/2021*

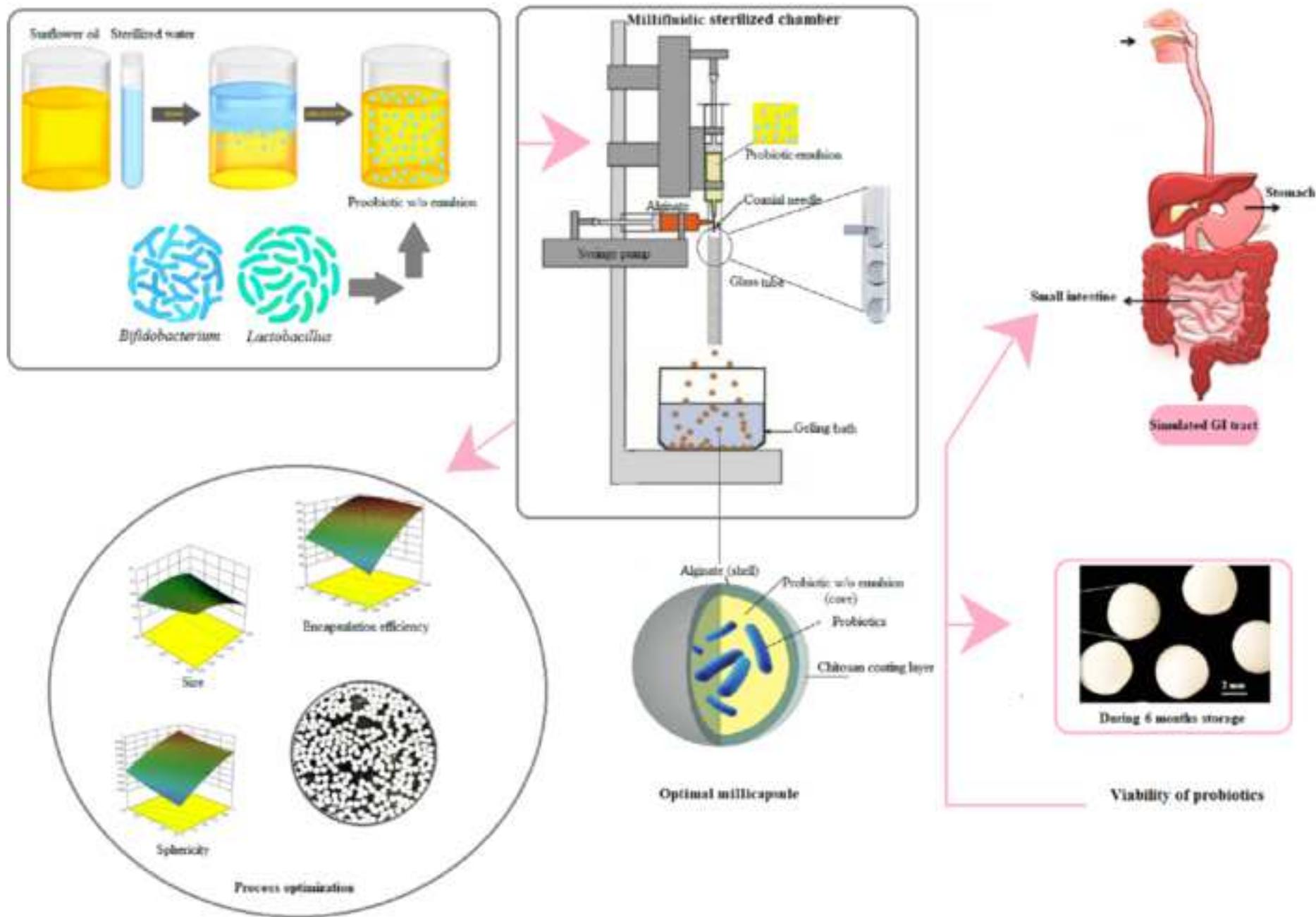
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## **Highlights**

- A millifluidic /direct gelation method was applied for encapsulation of probiotics.
- The central composite design was used for the optimization of the gelation process.
- The optimal emulsion-filled millicapsules had monodispersed spherical shapes.
- The survival efficiency of two encapsulated probiotic strains was higher than 90%.
- After 6 month storage at  $-18^{\circ}\text{C}$ , the number of live cells still met the standards.



1                   **A Millifluidic-assisted ionic gelation technique for encapsulation of**  
2                   **probiotics in double-layered polysaccharide structure**

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## Abstract

A unique double-layered probiotic delivery system based on a millifluidic/direct gelation method of encapsulation has been investigated. The effects of variation of alginate concentration (20-30 g/l), flow rates of alginate (0.8-1.2 ml/min), and water/oil (W/O) emulsion (0.5-0.7 ml/min) on emulsion encapsulation efficiency (EE), size, and sphericity (SF) of core-shell millicapsules were examined using a central composite design to optimize a delivery system for the encapsulated *Bifidobacterium animalis* subsp. *lactis* and *Lactobacillus plantarum*. The optimized calcium-alginate millicapsule was spherical ( $0.97 \pm 0.01$  SF), with an average diameter of  $4.49 \pm 0.19$   $\mu\text{m}$ , and an emulsion encapsulation efficiency of  $98.17 \pm 0.5\%$ . Two probiotic strains were encapsulated separately in W/O emulsion as a core of the millicapsule. After coating with chitosan, the encapsulation yield of the bacteria, survival rates under simulated gastrointestinal (GI) conditions, and viability during storage were determined. Survival efficiency values of *B. animalis* subsp. *lactis* and *L. plantarum* after millifluidic encapsulation were found to be 92.33 and 90.81%, respectively. Cell viability of probiotics embedded in the millicapsule after passing through the GI system was improved ( $7.5 \log \text{CFU ml}^{-1}$  for both strains). Although the viability of the encapsulated probiotics stored at  $-18 \text{ }^\circ\text{C}$  for six months significantly decreased ( $p < 0.05$ ), the number of live cells was approximately in accordance with the standard definition of long-term probiotic survival ( $6 \log \text{CFU g}^{-1}$ ).

**Keywords:** Millifluidic, Probiotics, Ionic gelation, Double-layered, In vitro digestion, Viability

## 53 1. Introduction

54 Probiotics are defined as living microorganisms that confer beneficial health effects on  
55 the host when administered in adequate amounts. Some positive effects of probiotics are the  
56 production of pathogen inhibitory substances, the prevention of adhesion of certain bacterial  
57 cells, toxin degradation, beneficial modulation of the gastrointestinal (GI) microbial flora, and a  
58 general enhancement of the immune system (Khaneghah, et al., 2020; Zhijing Liu, et al., 2020).  
59 To accomplish these beneficial functions, the probiotics must first survive being subject to  
60 variations in pH, oxidative conditions, and high temperature whilst processed into an edible  
61 form and then the harsh digestive conditions of the GI tract (acidity, bile salts, digestive  
62 enzymes), to reach the intestine in an appropriate quantity (Holkem, et al., 2016; Li, et al.,  
63 2019). Microencapsulation is an established technique to allow the survival of probiotics in food  
64 processing and formulations, and once through the GI tract, to promote their ability to colonize  
65 the mucosal surfaces (Anselmo, McHugh, Webster, Langer, & Jaklenec, 2016). However, very  
66 low or high temperatures, and/or organic agents that are part of common probiotic encapsulation  
67 techniques such as spray drying, freeze and fluid bed drying, and coacervation, lead to a  
68 considerable reduction in bacterial viability (Zaeim, et al., 2020), therefore alternative methods  
69 for drying and encapsulation of probiotics are desirable (Alehosseini, Sarabi-Jamab, Ghorani, &  
70 Kadkhodae, 2019).

71 Multilayer delivery systems have been proposed to improve the survival rate of  
72 encapsulated probiotics. Examples are the encapsulation of *Lactobacillus paracasei* BGP-1 in  
73 alginate/shellac by co-extrusion (Silva, et al., 2016), moist-heat-resistant multilayered  
74 microcapsules for encapsulation of *Lactobacillus acidophilus* (Pitigraisorn, Srichaisupakit,  
75 Wongpadungkiat, & Wongsasulak, 2017), encapsulation of *Lactobacillus acidophilus* in zein-

76 alginate core-shell microcapsules by electrospraying (Laelorspoen, Wongsasulak, Yoovidhya, &  
77 Devahastin, 2014) and the encapsulation of *Lactobacillus reuteri* in water/oil/water (W/O/W)  
78 double emulsions (Marefati, Pitsiladis, Oscarsson, Ilestam, & Bergenståhl, 2021). It is proposed  
79 that a double-layer delivery system could be developed using millifluidic encapsulation: this is a  
80 fast, straight forward, and cost effect manufacturing method that does not require toxic  
81 chemicals (Martins, Poncelet, Marquis, Davy, & Renard, 2017; Nativel, et al., 2018). Compared  
82 with conventional techniques such as extrusion or emulsification which generally have poor  
83 control of capsule diameter, the millifluidic method produces highly monodispersed droplets  
84 through precise control of the flow of both the dispersed and continuous phases. The  
85 hydrophobic core (an emulsion containing the probiotics) exists as a dispersed phase and the  
86 hydrophilic shell (sodium alginate solution) is a continuous phase and these are extruded into a  
87 tube. The double-layered droplets are formed by the shear forces between the two phases. Due  
88 to this opposition of forces the droplets fall into a gelling bath, and chemical interactions  
89 between the polymer chains and calcium ions produce a core-shell delivery system. Alginate as  
90 an anionic linear polysaccharide is degraded at a very low pH, therefore, the combination of this  
91 polymer with certain polycationic polymers such as chitosan leads to the formation of strong  
92 electrostatic repulsive forces between the amine and acid residues (Nualkaekul, Lenton, Cook,  
93 Khutoryanskiy, & Charalampopoulos, 2012). The millifluidic technique has been used for the  
94 production of emulsion oil-loaded capsules. According to Martins, et al. (2017), encapsulation  
95 of a W/O emulsion into capsules with the sizes ranging from 140  $\mu\text{m}$  to 1.4 mm was  
96 successfully achieved using the millifluidic/inverse gelation mechanism. Pereda, Poncelet, and  
97 Renard (2019) studied the influence of curing time and storage conditions on the  
98 physicochemical characteristics of the core-shell millicapsules produced by the

99 millifluidic/inverse gelation technique. Geometric, instrumental, and phases features of  
100 millifluidic/ dripping process were assessed for sunflower oil-loaded millicapsules (Farahmand,  
101 Emadzadeh, Ghorani, & Poncelet, 2021) who also examined flow pattern, droplet formation  
102 mechanism, and forces experienced by droplets inside the millifluidic device.

103 Recently, the millifluidic process has been extended to the microfluidic scale, which has  
104 been used for the cultivation of individual bacteria inside microfluidic double-layered emulsion  
105 droplets (Yoha, Nida, Dutta, Moses, & Anandharamakrishnan, 2021). A W/O emulsion of okara  
106 oil and block-copolymers of poly (acrylic acid) and Pluronic® has been used in a microfluidic  
107 device for the encapsulation of *Lactobacillus plantarum* (Quintana, et al., 2021).

108 To the best of our knowledge, despite of the advantages of millifluidic technique as an  
109 encapsulation process, no study has optimized this method for the encapsulation of probiotic  
110 bacteria. Therefore, in this study we aim to optimize the millifluidic technique for the  
111 encapsulation of two probiotic bacteria species, *Bifidobacterium animalis* subsp. *lactis* and  
112 *Lactobacillus plantarum*, separately, into optimal Ca-alginate/ chitosan millicapsules and to  
113 assess survival rates during storage and the viability of the encapsulated probiotics under  
114 simulated GI conditions.

## 115 **2. Materials and method**

### 116 **2.1. Materials, bacterial strains, and media**

117 Sunflower oil with a density of 918.8 kg/m<sup>3</sup> was provided by Nina Co, Iran, to make an  
118 emulsion with sterilized deionized water. Calcium chloride (CaCl<sub>2</sub>.2 H<sub>2</sub>O, 147.01 g/mol),  
119 sodium alginate (1.37 M/G ratio, 1.57× 10<sup>5</sup> g/mol, low viscosity), and low molecular chitosan  
120 powders were purchased (Sigma Aldrich, USA), and used as supplied. Surfactants (Tween 20  
121 with a hydrophilic–lipophilic balance (HLB) = 16.7 and PGPR 90 with HLB= 1.5) and glacial

122 acetic acid were also used as supplied (Merck, Germany). *Lactobacillus plantarum* PTCC  
123 1896<sup>TM</sup> (A7), was obtained from the microbial culture collection of IROST (Iranian Research  
124 Organization for Science and Technology, Tehran, Iran), and *Bifidobacterium animalis* subsp.  
125 *Lactis* (BB-12<sup>®</sup>) was purchased from Chr. Hansen (Hørsholm, Denmark). Both microorganisms  
126 were isolated as probiotic bacteria from the stool of breastfed babies. De Man, Rogosa and  
127 Sharpe (MRS) agar and broth, L-Cysteine hydrochloride, Anaerocult<sup>®</sup> A gas pack, hydrochloric  
128 acid, sodium hydroxide, potassium dihydrogen phosphate, and pepsin were obtained from  
129 Merck (Darmstadt, Germany). Tri-sodium citrate, bile salts, and pancreatin were supplied by  
130 Sigma-Aldrich (St. Louis, Missouri, USA).

131

## 132 **2.2. Methods**

### 133 **2.2.1. Activation of Probiotics**

134 To activate the lyophilized *Lactobacillus*, the A7 strain was propagated in MRS Broth  
135 medium and incubated at 37 °C for 18 h. BB-12<sup>®</sup> is an obligate anaerobic bacterium.  
136 Therefore, to create favorable conditions for lyophilized *Bifidobacterium*, 0.5 g/L L-Cysteine  
137 hydrochloride (Cys-HCl) was added to the MRS broth, and placed in an anaerobic jar with an  
138 Anaerocult<sup>®</sup> A gas pack at 37 °C for 24-48 h (Zaeim, Sarabi-Jamab, Ghorani, & Kadkhodae,  
139 2019).

140

### 141 **2.2.2. Water/Oil (W/O) emulsion preparation**

142 Preparation of W/O emulsion as the dispersed phase of millifluidic device was  
143 performed according to a modification of the method of Martins, et al. (2017). 80 ml of  
144 sunflower oil was mixed with 0.8 g PGPR 90 using a high shear mixer (Ultra-Turrax T25,

145 Germany) at 18000 rpm for 1 min. 20 ml of sterilized deionized water was then added drop wise  
146 and mixed at 18000 rpm for 2 min. About  $10^{10}$  CFU  $g^{-1}$  activated probiotic cells were harvested  
147 by centrifugation (Hermle Z-32 HK, Germany) at  $3500\times g$  and  $4\text{ }^{\circ}C$  for 10 min and the pellets  
148 were immediately washed thoroughly with sterilized distilled water to eliminate any residual  
149 MRS broth. Finally, 1 g of probiotic cells were dissolved in 1 ml sterilized deionized water,  
150 dispersed separately to 99 ml of emulsion, and mixed gently using a magnetic stirrer (IKA-RCT  
151 basic, Germany) at room temperature for 30 min to make homogeneous feed solutions. 1 ml  
152 samples were taken to count viable probiotics in the initial solution. It should be noted that the  
153 addition of bacterial pellets to the W/O emulsion was performed in sterile conditions.

### 154 **2.2.3. Preparing alginate, chitosan and calcium chloride solutions**

155 The calcium chloride solution used as the gelling bath was prepared by dissolving 30 g  
156 of powder in 1 liter of sterilized deionized water. Different concentrations of sodium alginate  
157 (20, 25, 30 g/L) were also made up using sterilized distilled water. After 24 h hydration, 6 g/L  
158 Tween 20 was added to the alginate solutions to reduce surface tension when forming the  
159 alginate droplet. Chitosan powder (15 g/L) was mixed with sterilized water containing 0.1 M  
160 acetic acid. After adjusting the pH to 5.5, the coating solution was continuously agitated for 1  
161 hour using a magnetic stirrer.

### 162 **2.2.4. Characterization of emulsion, and alginate solutions**

#### 163 **2.2.4.1. Emulsion stability**

164 The stability of the W/O emulsion was assessed by centrifugation and calculating the  
165 weight of the supernatant. Freshly formed emulsion ( $M_0$ ) was centrifuged at 5000 rpm for 10 min  
166 (Sciarini, Maldonado, Ribotta, Pérez, & León, 2009). After separating the supernatant part ( $M_1$ ),

167 stability of the emulsion was determined as a ratio of supernatant to the initial weight of the  
168 emulsion (**Eq. 1**).

$$169$$
$$170 \quad \text{ES (\%)} = (M_1/M_0) \times 100 \quad (1)$$
$$171$$

#### 172 **2.2.4.2. Flow behavior of emulsion and alginate solutions**

173 Viscosity of emulsion and alginate solutions at shear rates of 1-295 ( $\text{s}^{-1}$ ) were determined  
174 at 25 °C using a rotary viscometer (RVDV-II, Brookfield, USA) with an SC-18 spindle. The flow  
175 curves were fitted to the Power-law model according to **Eq. (2)**, where  $\sigma$  is the shear rate,  $n$  is the  
176 flow behavior index,  $K$  is the consistency coefficient, and  $\gamma$  is the shear rate.

$$177 \quad \sigma = K \cdot \gamma^n \quad (2)$$

178 Simulated shear rates of samples in the glass tube were calculated as follows (**Eq. 3**) (Wohl,  
179 1968), and the viscosities were determined at these shear rates.

$$180 \quad \gamma = \left(3 + \frac{1}{n}\right) Q / \pi r^3 \quad (3)$$

181 where  $Q$ ,  $r$ ,  $n$ , and  $\gamma$  are the flow rate of the continuous phase ( $\text{m}^3/\text{s}$ ), the inner radius of tube (m),  
182 flow behavior index, and simulated shear rate ( $\text{s}^{-1}$ ), respectively.

#### 183 **2.2.5. Millifluidic encapsulation of W/O emulsion**

184 A millifluidic device with coaxial geometry was made (Farahmand, et al., 2021; Martins,  
185 et al., 2017). The W/O emulsion as the dispersed phase was pumped (New Era, NE-300, USA)  
186 using a Teflon tube (interior and outside diameters: ID=0.6 and OD= 1.5 mm) at flow rates of  
187 0.5- 0.7 ml/min. A larger Teflon tube (ID= 0.9 and OD= 2 mm) was used to pump an alginate-  
188 Tween solution as continuous phase at flow rates of 0.8- 1.2 ml/min. The droplets were

189 generated by co-flowing the two phases in a glass tube (ID= 3.2, OD= 5 mm, length: 20 cm) to  
190 exert shear forces between phases. The pinched-off droplets were collected under sterilized  
191 conditions in the gelling bath (CaCl<sub>2</sub> 30 g/L) and stirred at 50 rpm for 30 min, then suspended in  
192 15 g/L chitosan solution for 15 min. After rinsing with sterilized water, the coated millicapsules  
193 were stored in sterilized bottles suspended in 15 g/L CaCl<sub>2</sub> solution at 4 °C.

194

## 195 **2.2.6. Characterization of the millicapsules**

### 196 **2.2.6.1. Dimensions and sphericity**

197 The sizes of at least 20 millicapsules were measured using Image J software (USA) and  
198 sphericity factors (SF) were calculated from this data. A digital microscope (Dino-lite pro,  
199 Taiwan) was used to capture all experimental runs (1280×1024 resolution and ×30  
200 magnification), the SF values were calculated as below (Davarcı, Turan, Ozcelik, & Poncelet,  
201 2017) (**Eq. 4**):

$$202 \quad SF = (2 d_{\min}) / (d_{\max} + d_{\min}) \quad (4)$$

203 Where d denotes the millicapsule diameter. The SF values above 0.95 confirm a spherical  
204 shape, and 0.9 < SF < 0.95 implied the oval and pear shape.

205

### 206 **2.2.6.2. Efficiency of emulsion encapsulation (EE)**

207 The amount of non-encapsulated emulsion was determined by collecting the  
208 millicapsules from the gelling bath and rinsing them three times with sterilized distilled water on  
209 a sieve covered with a filter paper (Whatman 41). After drying the filter paper in an oven  
210 (Binder-FP53, Germany) (105 °C) to constant weight, the EE was calculated as the difference

211 between the initial weight of the emulsion ( $W_i$ ), and that of the non-encapsulated emulsion ( $W_{ne}$ )  
212 (Eq. 5) (Chan, 2011):

213

$$214 \quad EE (\%) = (W_i - W_{ne}) / W_i \times 100 \quad (5)$$

### 215 **2.2.7. The survival efficiency of encapsulated probiotics**

216 The encapsulation efficiency of the probiotics was validated based on the number of  
217 viable cells before and after the millifluidic encapsulation process using a plate count method,  
218 and the percentage of surviving bacteria was calculated as follows:

$$219 \quad EY = \left( \frac{\log_{10} N}{\log_{10} N_0} \right) * 100 \quad (6)$$

220 where  $N$  and  $N_0$  are the number of cells in the millicapsules and in the initial feed solution  
221 (CFU g/1) (Haghshenas, et al., 2015; Heidebach, Först, & Kulozik, 2010).

222 To count the live cells before encapsulation, the feed solution containing viable cells was  
223 serially diluted in Ringer's solution (pH 7.0), plated, incubated, and counted. After  
224 encapsulation, the millicapsules were decomposed in 50 mM sodium citrate solution. Then  
225 the quantity of released live cells were estimated as described above.

226

### 227 **2.2.8. Bacterial survival under simulated gastrointestinal conditions**

228 To make the simulated gastric fluid, 3.2 g/L pepsin in 2 g/L NaCl solution was dissolved  
229 and the pH of the solution was adjusted to 2.5 by using 1 and 5 M HCl. Simulated intestinal  
230 fluid was prepared by dissolving 1 g/L pancreatin and 20 g/L bile salts in 0.1 mol/L potassium

231 dihydrogen phosphate solution, and finally, pH of the solution was adjusted to pH7.4 by 0.1 and  
232 1 M NaOH. Both the simulated gastric and intestinal solutions were then sterilized by a 0.2 µm  
233 cellulose acetate syringe filter and pre-warmed to 37 °C using a shaker water bath. 1 g of  
234 millicapsule solution was added to glasses containing 9 ml of simulated gastric fluid and  
235 agitated gently in a shaker incubator at 37 °C for 2 h. Following this step, using sterilized  
236 Whatman No. 4 filter paper, the millicapsules were separated from the simulated gastric  
237 solution and introduced into 9 ml of simulated intestinal fluid and stirred for at least 2 h under  
238 similar conditions (Annan, Borza, & Hansen, 2008; Cook, Tzortzis, Charalampopoulos, &  
239 Khutoryanskiy, 2011; Rao, Shiwnarain, & Maharaj, 1989). Sampling was performed every  
240 hour, and the number of live bacteria was determined by the plate count method. First, the  
241 millicapsules were entirely disintegrated in 50 mM sodium citrate solution for 15 to 30 min at  
242 room temperature on a shaker. After the bacteria were released from the millicapsule structure,  
243 a 1 ml sample was taken, serially diluted using sterile ringer solution, and then spread on MRS  
244 agar plates. Under at 37 °C incubation conditions the colonies appeared after 48-72 h. Bacterial  
245 count experiments were made in triplicate, and the data were presented as mean± standard  
246 deviation (Cook, et al., 2011; Heidebach, et al., 2010; Solanki, et al., 2013).

#### 247 **2.2.9. Viability of bacteria during storage time**

248 The millicapsules containing live probiotics were maintained at -18 °C for 6 months.  
249 The count of viable cells was determined monthly by the method described in the previous  
250 section.

251

252

## 253 2.2.10. Statistical analysis

254 The processing parameters, including alginate concentration ( $X_1$ , [Alg]: 20-30 g/l),  
255 the flow rate of alginate ( $X_2$ ,  $Q_{Alg}$ : 0.8-1.2 ml/min), and the flow rate of emulsion ( $X_3$ ,  
256  $Q_{emulsion}$ : 0.5-0.7 ml/min), were optimized by response surface methodology (RSM) with  
257 central composite design (CCD). In 20 experimental runs with 6 central points (**Table. 1**),  
258 characteristics of the millicapsules on the EE (Y1), size (Y2), and sphericity (Y3) were  
259 assessed. The data of dependent variables were fitted to a second-order polynomial equation  
260 (**Eq. 6**):

$$261 \quad Y = \beta_0 + \sum_{i=1}^n \beta_i X_i + \sum_{i=1}^{n-1} \sum_{j=i+1}^n \beta_{ij} X_i X_j + \sum_{i=1}^n \beta_{ii} X_i^2 \quad (6)$$

262 Where Y is the dependent variable,  $X_i$  and  $X_j$  are independent variables, and  $\beta_0$ ,  $\beta_i$ ,  $\beta_{ii}$ ,  $\beta_{ij}$  are  
263 regression coefficients. Optimization was analyzed by Design expert software (version 10,  
264 stat-Ease, USA) based on maximizing the EE, SF, and size.

265

266 **Insert Table. 1 about here**

267

268

269 Data analysis for bacterial survival under simulated gastrointestinal conditions and during  
270 storage at -18 °C, was carried out using the IBM® SPSS® software platform (version 20.0).  
271 One-way analysis of variance (ANOVA) was used to determine if there were significant  
272 ( $p < 0.05$ ) differences between sample means. Mean comparisons were performed using Duncan's  
273 Test. All the experiments were performed in triplicate, and the data were averaged and reported  
274 as mean  $\pm$  standard deviation.

### 275 3. Results and discussion

#### 276 3.1. Characterization of the continuous and dispersed phases

##### 277 3.1.1. Stability of the water/oil (W/O) emulsion

278 Monodispersed droplets have an effect on the stability of W/O emulsions, their  
279 controlled release, and physical characteristics such as viscosity, particle size, microstructure,  
280 and shape. In addition to processing parameters, emulsion compositions also have a significant  
281 impact on the long-term stability of W/O emulsions (Nisisako & Torii, 2008; J. Xu, Li, Tan,  
282 Wang, & Luo, 2006). In this research, W/O emulsion containing probiotics was selected as the  
283 dispersed phase of the millifluidic device, which must remain stable to protect the bacteria.  
284 Emulsion stability was assessed at 25 °C (room temperature) as a function of storage time (**Fig.**  
285 **1**) and centrifugal stability. As can be seen in **Fig.1**, it can be visually observed that our W/O  
286 emulsion as a carrier of probiotics was stable up to 36 h. Minimal phase separation and  
287 coalescence were observed during the storage time. According to our results, the centrifugal  
288 stability of W/O emulsion was 81.42%. This is because polyglycerol polyricinoleate (PGPR)  
289 could migrate quickly to the water/oil interface and form a structured interface that boosts steric  
290 hindrance thus playing a role in emulsion stability (Okuro, Gomes, Costa, Adame, & Cunha,  
291 2019). Therefore, reducing the interfacial tension between the two phases by using PGPR could  
292 simplify the fabrication of dispersed phase droplets at the junction of two fluids in the tube.  
293 These droplets are formed in tube through exerting the shear stress of the continuous phase on  
294 the dispersed phase (Costa, Gomes, Ushikubo, & Cunha, 2017).

295

296

**Insert figure.1 about here**

297

### 298 3.1.2. Flow behavior of phases

299 The flow behavior parameters of the continuous and dispersed phases at various  
300 concentrations and flow rates of the millifluidic device are reported in **Table .2**. The curve of  
301 viscosity versus shear rates of phases (data not shown) depicted shear-thinning (pseudoplastic)  
302 behavior of alginate solutions at three different concentrations. This behavior is also confirmed  
303 by Power-law model fitting (**Table. 2**) with a flow behavior index of less than 1 ( $n < 0.72$ ). The  
304 viscosity distribution of non-Newtonian fluids around a droplet in the tube depends on the shear  
305 rate, which could change the droplet size (Vagner, Patlazhan, & Serra, 2018). Hence, after  
306 calculating of the simulated shear rate in the tube according to **Eq. 3**, viscosity in the tube was  
307 also reported in **Table. 2**. It should be noted that as the alginate concentration was increased  
308 from 20 to 30 g/l, the viscosity also increased due to individual alginate molecules overlapping  
309 and forming intermolecular junctions (Funami, et al., 2009). The consistency coefficient (k) in  
310 continuous phase solutions also increased with increasing concentration (from  $317.6 \pm 0.9$  to  
311  $1853.08 \pm 1.07$  mP.s). Shear-thinning behavior is associated with cluster breakup and chain  
312 alignment, leading to viscosity reduction of solution during movement, so increasing the flow  
313 rate of solution favors the flow process (Costa, et al., 2017). The W/O emulsion showed a more  
314 pronounced Newtonian behavior (higher n value). The consistency index (k) and viscosity were  
315 also lower as compared with alginate solutions. Sunflower oil + PGPR showed Newtonian  
316 rheological behavior, that could be attributed to the long chain of triacylglycerols structure and  
317 chain unsaturation (Gomes, Costa, & Cunha, 2018; Meirelles, et al., 2021).

318 The viscosities of both phases are important from two aspects: first, viscosity shows an  
319 impact on the droplet size. For example, Guillot and Colin (2005) and Garstecki, Stone, and  
320 Whitesides (2005) reported a reverse effect of continuous phase viscosity on the droplet size.

321 Furthermore, increasing the dispersed phase viscosity will change both the squeezing pressure  
322 and the viscous shear which affect droplet detachment. More viscous liquid is pushed out of the  
323 tube before the collapse of the droplet neck. Slow breakup of the dispersed fluid results in large  
324 droplet formation. In other words, a larger shear force is needed to overcome the interfacial  
325 tension of the high viscosity dispersed phase (Zheyu Liu, Chai, Chen, Hejazi, & Li, 2021).  
326 Second, the continuous phase viscosity above 500 mPa.s, will cause problems both with  
327 pumping and the final shape of the millicapsules (Moghadam, Samimi, Samimi, & Khorram,  
328 2008). As shown in **Table. 2**, both phases at all simulated shear rates had viscosity values lower  
329 than the mentioned critical value. Also, viscosity value of the dispersed phase was lower than  
330 the continuous phase ( $Q_{Alg} > Q_{emulsion}$ ).

331

332

**Insert Table. 2 about here**

333

334

335

### 336 **3.2. Characterization of the millicapsules**

337 To study the effect of process variables (flow rates of two phases, and alginate  
338 concentration) on the millicapsule properties (encapsulation efficiency, size, and sphericity),  
339 ANOVA was used and confirmed the validity of the experimental design responses (see  
340 **Supplementary, Table. 1**). The fitted equations for each response were written in **Table. 3**.

341

342

343

**Insert Table. 3 about here**

### 344 **3.2.1. Effect of independent variables on EE**

345 High encapsulation efficiency (EE) is the main advantage in production of larger capsules  
346 (Chen, Li, Liu, & Meng, 2017). The larger capsules enable greater protection to the core, due to  
347 the reduced rate of core penetration of oxygen (Silva, et al., 2018), and by providing an effective  
348 barrier against harsh conditions. Significant interactions among the variables affecting EE are  
349 shown in **Fig. 2, A-C**. As shown in **Fig. 2 (A)**, the addition of the alginate flow rates (0.8 to 1.2  
350 ml/min) could improve the EE of W/O emulsion from  $37.5 \pm 0.2$  to  $62.15 \pm 0.56\%$ .

351 The distance between detached droplets from the millifluidic tube and droplet size can be  
352 controlled by tuning flow rates. The effect of forces exerted on the droplets in the millifluidic  
353 tube (Farahmand, et al., 2021), relate to increasing the flow rate of the continuous phase leading  
354 to higher pressure on the interface, higher velocity gradient, and consequently higher viscous  
355 forces, which may break the dispersed phase (W/O emulsion) into droplets inside the millifluidic  
356 tube. The time required for the detachment of droplets from the tube will be shortened.  
357 Subsequently, a lower volume fraction of fluid in the droplet leads to a reduction in size and to  
358 complete covering by the continuous phase (Cramer, Fischer, & Windhab, 2004; Fu, Wu, Ma, &  
359 Li, 2012). The differences between the viscosity and flow rates of both phases led to an increase  
360 in intromission of the alginate phase (shell) into the detached droplets compared to the case when  
361 a W/O emulsion dispersed phase forms the core. This higher shell/core ratio caused a thicker  
362 shell in the millicapsule due to more interactions of alginate and calcium ions, hence becoming  
363 more effective in entrapping the emulsion core (higher EE).

364 Regarding the EE (**Fig. 2, B**), it was possible to establish an inverse relationship between  
365 flow rate of the W/O emulsion and EE. More resistance to the continuous phase induced at  
366 higher flow rates of the dispersed phase led to larger droplets. Benavides, Cortés, Parada, and

367 Franco (2016) also observed this trend in capsules of thyme essential oil produced by ionic-  
368 gelation, noting that entering a higher amount of oil as dispersed phase led to the presence of a  
369 significant amount near the capsule surface due to limitation of capsule capacity. This thin  
370 shelled overloaded capsule could not maintain a core in the gelling bath, so the EE was  
371 decreased. A significant interaction between flow rates of the continuous phase and the dispersed  
372 phase is shown in **Fig. 2 (C)**.

373 As demonstrated in **Fig. 2 (A, B)**, augmenting the alginate concentration (and hence  
374 viscosity) from 20 to 30 g/l led to higher EE values (from  $61.53 \pm 0.74$  to  $98.9 \pm 0.25$  %). Greater  
375 availability of active sites in the alginate chains could bind to  $\text{Ca}^{2+}$  and with higher degree of  
376 cross-linking. Rousseau, Le Cerf, Picton, Argillier, and Muller (2004) show similar results  
377 showing that the alginate concentration has a considerable effect on the mesh size of capsules,  
378 with larger pore sizes created at lower concentrations of alginate. Hence, the movement of lipid  
379 droplets to the surface of porous capsules and also the surrounding aqueous medium is  
380 facilitated. This high leakage in the gelling step plays a role in the EE reduction: a higher  
381 concentration of the continuous phase induces higher detaching forces, which are exerted on the  
382 droplet at the tip of the tube (Martins, et al., 2017).

383

384 **Insert figure.2 about here**

385

386

387

388

### 389 3.2.2. Effect of independent variables on size

390 Droplet size and the millicapsule size directly determine the quality of the encapsulated  
391 compounds, the characteristics of produced emulsion, and the amount of oil recovery (C. Xu &  
392 Xie, 2017). The diameter of millicapsules varied from  $4.37 \pm 0.1$  to  $4.68 \pm 0.02$  mm at different  
393 experimental runs (**Fig. 2, D-F**). Cavaleiro, et al. (2019) also produced probiotic capsules with  
394 a millimeter scale. According to Chen, et al. (2017), macrocapsules contain a higher load of  
395 probiotics, increasing the EE.

396 The interaction of the flow rate and concentration (**Fig. 2, D**) showed that millicapsule  
397 size decreased in inverse proportion to the alginate flow rate ( $Q_{Alg}$ ) as it varied from 0.8 to 1.2  
398 ml/min. Droplets decrease in size when the velocity of the continuous phase increases because  
399 of the larger shear stress exerted on the interface (Lan, Jing, Guo, & Li, 2017). Cramer, et al.  
400 (2004) investigated the effect of flow rates, fluid viscosity, and interfacial tension on droplet  
401 size. Their results indicate that increasing the flow rate of the continuous phase means more  
402 efficient detachment from the tube, and consequently, a reduction in droplet size. Furthermore,  
403 the effect of shear stress on the continuous phase at higher flow rates could be more significant  
404 than interfacial tension between the dispersed phases (Meirelles, et al., 2021).

405 Significant interactions between the flow rate of the dispersed phase and concentration  
406 of the continuous phase (**Fig. 2, E**) are demonstrated by the steep slope of the plot of emulsion  
407 flow rate ( $Q_{emulsion}$ ), indicating the sensitivity of size to this parameter. It was found that the  
408 largest millicapsule ( $4.68 \pm 0.13$  mm) was obtained at  $Q_{emulsion}$  of 0.7 ml/min, due to the high  
409 loading of the emulsion into droplets compared to the alginate solution. Zheyu Liu, et al. (2021)  
410 and Amine, et al. (2020) examining millifluidic methods, also reported that an increase in flow  
411 rate of the dispersed phase led to increasing the droplet size, which they related to the

412 magnitude of shear and inertial forces. A similar trend is also shown in the three-dimensional  
413 interaction plot of the phases flow rates (**Fig. 2, F**).

414 It was found from **Fig. 2, D** that alginate concentration ([Alg]) had an adverse effect on  
415 the millicapsule diameter. Based on **Table. 2**, the higher concentration of continuous phase  
416 (with high viscosity in millifluidic tube) exerted a higher drag force on the dispersed phase and  
417 also quickly broke up the small droplets. This finding was in accordance with other millifluidic  
418 studies (Farahmand, et al., 2021; Martins, et al., 2017).

419

### 420 **3.2.3. Effect of independent variables on SF**

421 The minimal surface/volume ratio of spherical shapes results in a lower release rate of  
422 any loaded compounds. **Fig. 2 (G-I)** illustrates the three-dimensional response surface plots as  
423 a function of the continuous phase concentration and flow rates of both phases. As can be seen,  
424 there were significant interactions among the independent variables for response to sphericity  
425 factor (SF). SF values were in the range of 0.85-0.98, which indicated millifluidic method  
426 conditions that produce completely round capsules. As depicted in **Fig. 2 (G)**, the highest  
427 sphericity of millicapsules was obtained at an alginate flow rate of 1.2 ml/min. Furthermore,  
428 the favorable effect of alginate flow rate is amplified at higher alginate concentrations  
429 (SF=99.3). Increasing the alginate flow rate results in the high drag force. Consequently,  
430 detaching time of droplet is shortened, and lower fluid accumulation produces smaller droplets  
431 (Lee, Ravindra, & Chan, 2013). According to the momentum equation (Momentum=mass×  
432 velocity), when two droplets fall from the same height, the smaller one has less momentum (ie  
433 impulse at collision). Therefore, smaller droplets are obtained at higher alginate flow rates.

434 **Fig. 2 (H, I)** shows that the W/O emulsion flow rate had an inverse effect on sphericity.  
435 By immersing the droplet in the gelling bath, viscous forces within the droplet retain the  
436 spherical shape while drag forces induced via the bath tend to disrupt the capsule. As the flow  
437 rate of the dispersed phase was increased, larger droplets with thinner shells were obtained.  
438 These droplets either could not tolerate the forces experienced inside the gelling bath, or were  
439 disintegrated on the surface due to high momentum.

440 In **Fig. 2 (H)**, we can see that more spherical millicapsules were formed at higher  
441 concentrations of alginate. There is a direct relationship between penetration depth into the  
442 gelling bath and sphericity of capsules. Higher droplet viscosity allows a more spherical  
443 shape to form as a result of deeper penetration (Davarcı, et al., 2017). Moreover, a strong  
444 network-like structure is made from an increase in cross-linking reactions within the high  
445 viscous droplets, improving the shape of the millicapsule.

446

#### 447 **3.2.4. Optimization of the millifluidic process and model validation**

448 Optimized amounts of  $[Alg]= 30g/l$ ,  $Q_{Alg}= 1.2$  ml/min, and  $Q_{emulsion}= 0.5$  ml/min to  
449 achieve the maximum EE (99.34%), size (4.42 mm), and SF (0.98) were obtained using the  
450 numerical point prediction method. The target accuracy criterion was 0.92. The reliability of  
451 predicted optimized conditions was tested with a series of experiments using the optimized  
452 variables, and the results were measured as  $98.17 \pm 0.5\%$ ,  $4.49 \pm 0.19$  mm, and  $0.97 \pm 0.01$ . These  
453 results agreed with the corresponding predicted values and confirmed the high accuracy of the  
454 models in predicting the millifluidic process. **Fig. 3** depicts the calcium-alginate millicapsules  
455 with W/O emulsion core covered with a chitosan shell, corroborating the proper application of  
456 the millifluidic method to achieve emulsion-filled delivery system. The analysis of millicapsule

457 revealed spherical shape with uniform size, smooth surface, and emulsion distributed  
458 throughout the matrix.

459

460

461

**Insert figure.3 about here**

462

463

464

### 465 **3.3.Evaluation of encapsulated probiotic efficiency at the optimized conditions**

466 During encapsulation, probiotic cells are often exposed to the environmental challenges,  
467 such as oxygen, thermal, mechanical stresses or severe acidic conditions in the stomach that may  
468 affect cell viability and proliferation. Therefore, depending on the encapsulation method and the  
469 amount of stress applied during it, the encapsulation efficiency of probiotics will vary (Okuro,  
470 Thomazini, Balieiro, Liberal, & Fávaro-Trindade, 2013; Sathyabama & Vijayabharathi, 2014).

471 The cell live number of *Lactobacillus plantarum* and *Bifidobacterium animalis* in the  
472 initial feed solution was  $10.08 \pm 0.07$  and  $10.56 \pm 0.04$  CFU g<sup>-1</sup>, respectively. After millifluidic  
473 process, the number of viable cells was dropped to  $9.31 \pm 0.05$  Log CFU g<sup>-1</sup> for *Lactobacillus*  
474 *plantarum* and  $9.59 \pm 0.06$  Log CFU g<sup>-1</sup> for *Bifidobacterium animalis*. Tests indicate that less  
475 than 1 log cycle of *Lactobacillus plantarum* and about 1 log cycle of *Bifidobacterium animalis*  
476 were either inactivated or lost into the collector solution during the millifluidic encapsulation  
477 method. However, the survival efficiency of A7 and BB-12® was found to be close to 92.36%  
478 and 90.81%. The encapsulation efficiency of probiotics is generally in the range of 60-95% and  
479 an EE value greater than 90% has rarely been reported (Pitigraisorn, et al., 2017; Silva, et al.,  
480 2016), so the encapsulation technique and operational conditions play a key role in achieving

481 high encapsulation efficiency (Y. Liu, Sun, Sun, & Wang, 2016; Pitigraisorn, et al., 2017; Shi,  
482 et al., 2013).

### 483 **3.4. Effect of the millifluidic encapsulation on viability of probiotics under the simulated GI** 484 **conditions**

485 After the exposure of encapsulated *Lactobacillus plantarum* (A7) and *Bifidobacterium*  
486 *animalis* subsp. *lactis* (BB-12®) to simulated gastric fluid, the number of live bacteria in both  
487 samples decreased by about one logarithmic cycle (**Table. 4**). The results also showed that after  
488 2 h of exposure of the encapsulated A7 to simulated gastric conditions, less than one other  
489 logarithmic cycle in the number of live bacteria was observed, while for BB-12®, more than one  
490 logarithmic cycle decreased. This effect can be attributed to the diffusion of small hydrogen ions  
491 (H<sup>+</sup>) from the simulated gastric fluids into the microgels that deactivate the probiotic cells  
492 (Zhang, et al., 2021).

493 By transferring the samples to simulated intestinal fluid and incubating for 2 h, it was  
494 observed that the live cell number in both samples did not decrease; In other words, the  
495 millifluidic encapsulated microorganisms tolerated the harsh conditions of the simulated  
496 intestinal environment (particularly the presence of bile salts and the pancreatin), and their  
497 viability remained almost constant. In some cases, an increase in the growth rate of bacteria was  
498 observed, which can be attributed to the adaptation of the microorganism to the simulated  
499 conditions of the intestine, as well as the use of bile salts as a nutrient source.

500 Finally, the results showed that when *Lactobacillus plantarum* was exposed to simulated  
501 GI conditions for 4 h, approximately 7.50 log CFU mL<sup>-1</sup> of bacteria survived. For  
502 *Bifidobacterium animalis* subsp. *Lactis*, at the end of the time of exposure to simulated  
503 conditions of the GI tract, the number of live cells was about 7.54 log CFU mL<sup>-1</sup>. This section

504 showed that the encapsulation of probiotic bacteria in the alginate-chitosan millicapsule  
505 improves the viability of cells as it passes through the GI tract. These results are also in the line  
506 with previous publications on the development of core-shell microencapsulation systems  
507 (Laelorspoen, et al., 2014; Silva, et al., 2016; Zhang, et al., 2021) as well as W/O microfluidic  
508 emulsions for encapsulation of probiotics (Quintana, et al., 2021).

509

510

511 **Insert Table. 4 about here**

512

513

### 514 **3.5. Effect of the millifluidic encapsulation on the viability of probiotics during storage**

515 One of the most critical factors in encapsulating of bioactive compounds such as  
516 probiotic bacteria is their stability during storage. Therefore, role of the millifluidic  
517 encapsulation method as well as biopolymers forming the capsule wall in maintaining the  
518 survival of probiotic bacteria during shelf-life was investigated. It should be noted that the  
519 loading of probiotics within the millicapsule has a direct effect on their survival rate during  
520 passage through the simulated GI tract and storage time. In this study, the initial number of both  
521 *Lactobacillus plantarum* and *Bifidobacterium animalis* subsp. *Lactis* live cells before  
522 encapsulation were about 10 log CFU mL<sup>-1</sup>.

523 **Table. 5** shows the number of surviving encapsulated probiotics when stored at -18 °C  
524 for six months. As can be seen, the survival of both bacteria decreased by about 4 logarithmic  
525 cycles. Concerning to *Lactobacillus plantarum*, the number of viable cells after production was  
526 about 9 log cycles, indicating a reduction of about 1 log cycle during the millifluidic

527 encapsulation process. By the end of the first month of storage, there was only a decrease of one  
528 log cycle compared to the initial number of microorganisms; However, viable counts remained  
529 almost unchanged in the millicapsule after the second month. Meanwhile, during the third and  
530 fourth months, the viable cells were reduced from  $8.07 \pm 0.23$  to about 7 log CFU g<sup>-1</sup>, and in the  
531 fifth and sixth months, the number of living bacteria reached  $6.39 \pm 0.07$  and  $5.41 \pm 0.08$  Log  
532 CFU g<sup>-1</sup>, respectively. In other words, the survival rate of millifluidic encapsulated  
533 *Lactobacillus plantarum* is acceptable only until the end of the fifth month, which is considered  
534 acceptable according to the standards defined for probiotic products that have been  
535 recommended that food products should contain 6 Log CFU g<sup>-1</sup> or more viable probiotics to  
536 exhibit their beneficial health effects (Zhang, et al., 2021).

537         Regarding the survival of *Bifidobacterium animalis* subsp. *Lactis* during six-month  
538 shelf-life tests (**Table. 5**), on the first day of counting (initial number after production), the  
539 number of millifluidic encapsulated bacteria was more than 9 logarithmic cycles. After one  
540 month of storage, the live cells were reduced by about one logarithmic cycle: the number of  
541 surviving *Lactobacillus plantarum* was  $8.36 \pm 0.14$  Log CFU g<sup>-1</sup>. The number of live cells of  
542 BB-12® remained about 7 log cycles until the end of the fourth month of storage and reached  
543 about 6, and 5 log cycles in the fifth, and sixth months.

544         The results of the survival study during the storage time of two probiotics (A7 and BB-  
545 12®) encapsulated by millifluidic method showed a significant decrease over time ( $p < 0.05$ ).  
546 However, after 5 months of storage, their number of live cells per gram of capsule was still in  
547 accordance with the standard definition of probiotics. A similar pattern of reduction in the  
548 viability of probiotics during the storage was also reported by Silva, et al. (2016) for *L.*  
549 *paracasei* BGP-1 incorporated sunflower oil or coconut fat matrix and co-extruded with

550 alginate-shellac blend, Silva, et al. (2018) for *L. acidophilus* LA3 co-extruded by the blend of  
551 alginate-shellac, and Zhang, et al. (2021) for *Bifidobacterium pseudocatenulatum* G7 co-  
552 encapsulated within calcium alginate microgels, colloidal antacid and nano-emulsion lipid  
553 droplets.

554

555 **Insert Table. 5 about here**

556

### 557 **3.6. Conclusion**

558 Millifluidic/direct gelation method was applied as a platform to produce the W/O  
559 emulsion-filled millicapsule for encapsulation of two probiotic bacteria: *Bifidobacterium*  
560 *animalis* subsp. *lactis* and *Lactobacillus plantarum*. The effect of process variables on  
561 morphology, size, and encapsulation efficiency of millicapsule was studied. Optimal emulsion-  
562 filled millicapsules had uniform spherical shapes of monodispersed size. A high efficiency of  
563 bacterial survival was achieved after the encapsulation process (reduction about one log cycle).  
564 The millicapsules also strongly protected both strains against the simulated GI conditions. The  
565 numbers of live cells were still in accordance with the standard definition of probiotics after six  
566 months of storage. Accordingly, the utility of the millifluidic encapsulation method paves the  
567 way for fabrication of a unique carrier for probiotic bacteria. Furthermore, encapsulation of  
568 lipophilic compounds in the oil part and hydrophilic compounds in the water part of emulsion  
569 loaded in millicapsules can be exploited co-encapsulation in various domains, an advance which  
570 needs further investigation.

571

572

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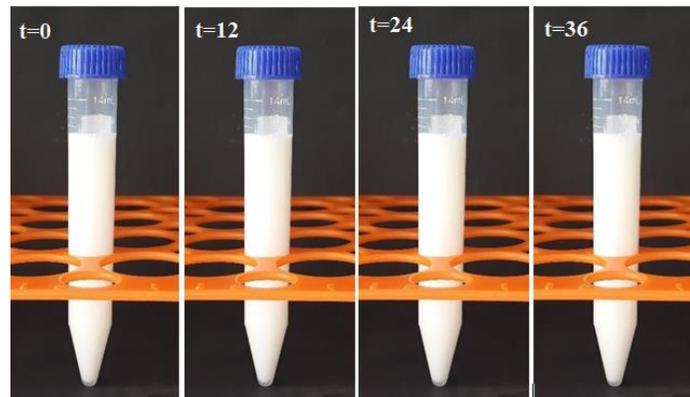
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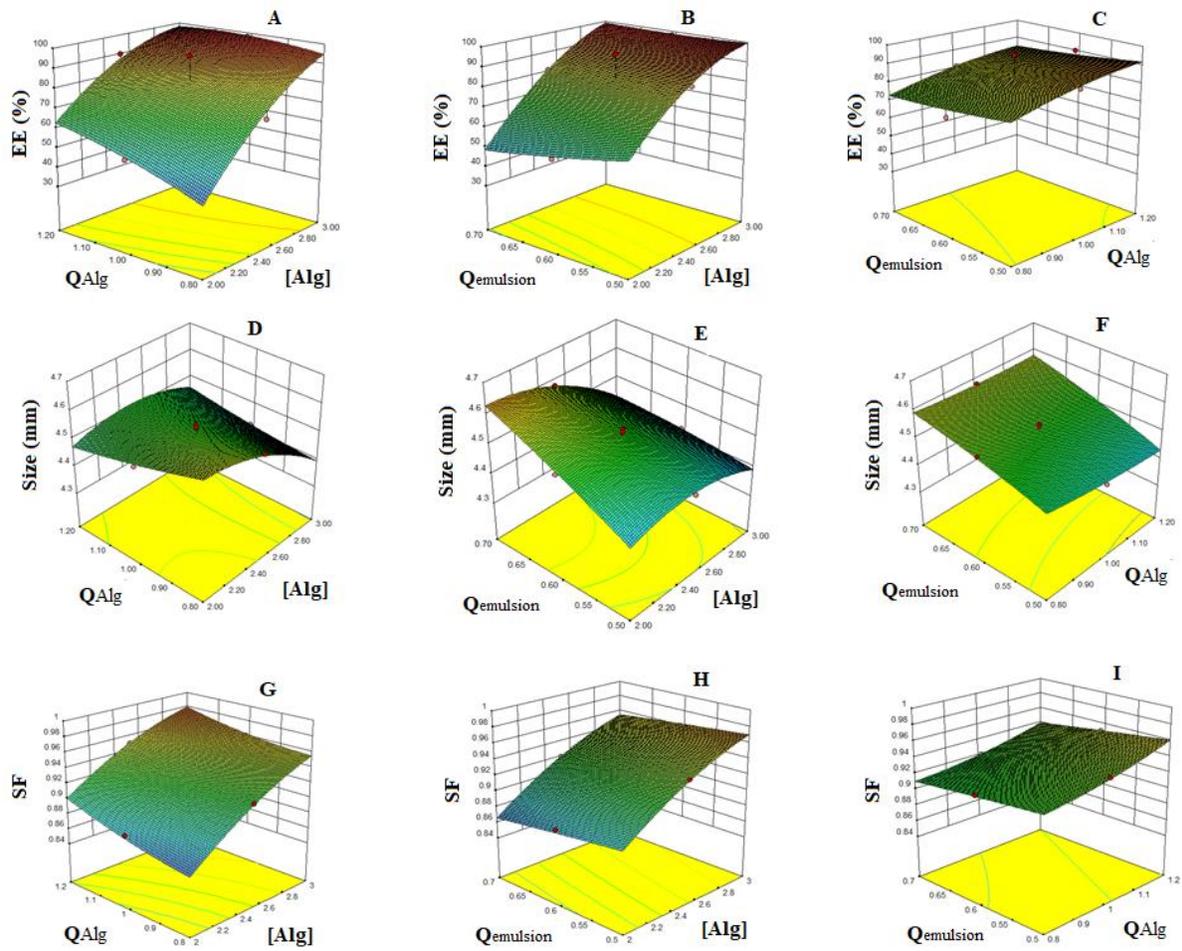
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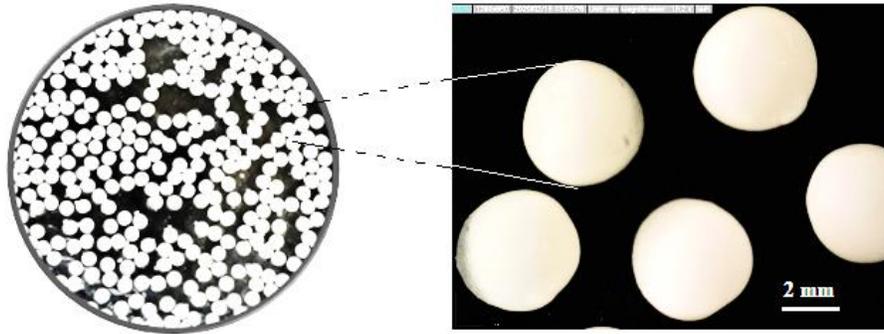
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**Figures:**

**Fig. 1.** Stability of W/O emulsion containing probiotics during 36 h storage time



**Fig. 2.** Three-dimensional plots of the response surfaces for EE (A-C), Size (D-F), and SF (G-I) as a function of interactions between concentration and flow rates of the alginate (A, D, G), alginate concentration and flow rate of emulsion (B, E, H), and flow rates of the emulsion and alginate (C, F, I).



**Fig 3.** Digital microscopic images of the emulsion-filled millicapsule produced at the optimized conditions ( $[Alg]: 30 \text{ g/l}$ ,  $Q_{Alg}: 1.2 \text{ ml/min}$ ,  $Q_{emulsion}: 0.5 \text{ ml/min}$ ) of the millifluidic encapsulation

**Tables:****Table 1.** Coded and uncoded factors for RSM were ascertained from 20 experimental runs of CCD design.

Run	Uncoded variables			Coded variables		
	[Alg], (g/l)	Q <sub>Alg</sub> , (ml/min)	Q <sub>emulsion</sub> , (ml/min)	X <sub>1</sub>	X <sub>2</sub>	X <sub>3</sub>
1	25	1.2	0.6	0	+1	0
2	25	1	0.6	0	0	0
3	30	1.2	0.5	+1	+1	-1
4	25	1	0.7	0	0	+1
5	25	1	0.5	0	0	-1
6	20	1.2	0.5	-1	+1	-1
7	25	1	0.6	0	0	0
8	25	1	0.6	0	0	0
9	20	1.2	0.7	-1	+1	+1
10	25	0.8	0.6	0	-1	0
11	20	0.8	0.7	-1	-1	+1
12	20	1	0.6	-1	0	0
13	30	1.2	0.7	+1	+1	+1
14	30	1	0.6	+1	0	0
15	30	0.8	0.7	+1	-1	+1
16	20	0.8	0.5	-1	-1	-1
17	25	1	0.6	0	0	0
18	25	1	0.6	0	0	0
19	30	0.8	0.5	+1	-1	-1
20	25	1	0.6	0	0	+1

**Table 2.** Rheological parameters of the continuous (alginate solutions) and dispersed phases (W/O emulsion) in the power-law model and viscosity at the simulated shear rate in the millifluidic tube

Phase	Power-law model				Flow rate (ml/min)	Simulated shear rate (1/s)	Viscosity at the simulated shear rate (mP.s)
	k	n	R <sup>2</sup>	RMSE			
W/O emulsion	0.77± 0.02 <sup>d</sup>	0.96± 0.01 <sup>a</sup>	0.99	0.02	0.5	2.6 <sup>h</sup>	76.13± 0.66 <sup>h</sup>
					0.6	3.15 <sup>g</sup>	87.18± 0.84 <sup>g</sup>
					0.8	3.78 <sup>g</sup>	89.14± 0.47 <sup>g</sup>
Alg 20	317.6± 0.9 <sup>c</sup>	0.72± 0.03 <sup>b</sup>	0.99	0.31	0.8	4.42 <sup>f</sup>	114.61± 0.23 <sup>f</sup>
					1	5.44 <sup>d</sup>	115.82± 1.03 <sup>f</sup>
					1.2	6.81 <sup>b</sup>	118.60± 0.40 <sup>f</sup>
Alg 25	486.72± 1.6 <sup>b</sup>	0.68± 0.06 <sup>c</sup>	0.99	0.18	0.8	4.51 <sup>f</sup>	157.75± 1.11 <sup>e</sup>
					1	5.54 <sup>d</sup>	162.15± 1.09 <sup>d</sup>
					1.2	6.92 <sup>b</sup>	165.71± 0.59 <sup>d</sup>
Alg 30	1853.08± 1.07 <sup>a</sup>	0.56± 0.02 <sup>d</sup>	0.98	0.09	0.8	4.82 <sup>e</sup>	401.94± 1.47 <sup>c</sup>
					1	5.92 <sup>c</sup>	416.53± 1.91 <sup>b</sup>
					1.2	7.41 <sup>a</sup>	431.42± 1.08 <sup>a</sup>

Values represent means ± SD (number of test repetitions= 3).

Different letters within the same column show significant differences (p < 0.05).

**Table 3.** Second-ordered quadratic models developed for EE, size and SF

<b>Responses</b>	<b>Predicted models</b>	<b>R<sup>2</sup></b>	<b>R<sup>2</sup><sub>adj</sub></b>	<b>covariance</b>	<b>Adequate precision</b>
<b>EE</b>	$Y_1 (\text{EE}) = 83.63 - 22.06 X_1 - 6.15 X_2 - 3.34 X_3 - 4.42 X_1 X_2 + 3.25 X_1 X_3 - 0.11 X_2 X_3 - 7.11 X_1^2 - 2.14 X_2^2 + 0.74 X_3^2$	0.97	0.97	5.31	21.16
<b>Size</b>	$Y_2 (\text{size}) = 4.52 - 0.054 X_1 - 0.01 X_2 + 0.06 X_3 + 0.04 X_1 X_2 - 0.04 X_1 X_3 + 0.01 X_2 X_3 - 0.05 X_1^2$	0.92	0.93	0.25	41.12
<b>SF</b>	$Y_3 (\text{SF}) = 0.93 + 0.043 X_1 + 0.016 X_2 - (9 \times 10^{-3}) X_3 - (3.75 \times 10^{-3}) X_1 X_2 + (1.25 \times 10^{-3}) X_1 X_3 - (1.25 \times 10^{-3}) X_2 X_3 - 0.01 X_1^2 + (4.54 \times 10^{-3}) X_2^2 - (4.5 \times 10^{-4}) X_3^2$	0.99	0.99	0.22	95.35

**Table 4.** Survival of the encapsulated probiotics in the simulated gastrointestinal fluids

Type of microorganism	Initial number of live cells after encapsulation process (Log CFU mL <sup>-1</sup> )	Number of live bacteria in the simulated gastric fluid (Log CFU mL <sup>-1</sup> )			Number of live bacteria in the simulated intestinal fluid (Log CFU mL <sup>-1</sup> )		
		The moment of entering the fluid	After 1 hour	After 2 hours	The moment of entering the fluid	After 1 hour	After 2 hours
<i>Lactobacillus plantarum</i>	9.31±0.05* <sup>Aa**</sup>	8.37±0.21 <sup>Bb</sup>	8.49±0.15 <sup>Ab</sup>	7.97±0.12 <sup>Ac</sup>	7.46±0.16 <sup>Ad</sup>	7.80±0.04 <sup>Ac</sup>	7.50±0.19 <sup>Ad</sup>
<i>Bifidobacterium animalis</i>	9.59±0.06 <sup>Ba</sup>	8.72±0.12 <sup>Ab</sup>	8.24±0.23 <sup>Ac</sup>	7.39±0.09 <sup>Bde</sup>	7.17±0.15 <sup>Ac</sup>	7.26±0.16 <sup>Bc</sup>	7.54±0.08 <sup>Ad</sup>

\* mean ± standard deviation (n=3)

\*\*Different capital letters in each column indicate the significant differences (p<0.05).

\*\*Different small letters in each row indicate the significant differences (p<0.05).

**Table 5.** Survival of the encapsulated probiotics during storage (log CFU g<sup>-1</sup>)

Sampling time	Type of microorganism	
	<i>Lactobacillus plantarum</i>	<i>Bifidobacterium animalis</i>
After encapsulation process	9.43±0.01* Aa**	9.37±0.28 <sup>Aa</sup>
After 1 month	8.59±0.03 <sup>Ba</sup>	8.36±0.14 <sup>Bb</sup>
After 2 months	8.07±0.23 <sup>Ca</sup>	7.64±0.01 <sup>Cb</sup>
After 3 months	7.39±0.00 <sup>Db</sup>	7.61±0.12 <sup>Ca</sup>
After 4 months	7.00±0.29 <sup>Ea</sup>	7.16±0.07 <sup>Da</sup>
After 5 months	6.39±0.07 <sup>Fb</sup>	6.67±0.15 <sup>Ea</sup>
After 6 months	5.41±0.08 <sup>Ga</sup>	5.49±0.09 <sup>Fa</sup>

\* mean ± standard deviation (n=3)

\*\*Different capital letters in each column indicate the significant differences (p<0.05).

\*\*Different small letters in each row indicate the significant differences (p<0.05).

## Conflict of Interest Disclosure Statement

We wish to confirm that there are no known conflicts of interest associated with this publication and there has been no significant financial support for this work that could have influenced its outcome.

We confirm that the manuscript has been read and approved by all named authors and that there are no other persons who satisfied the criteria for authorship but are not listed. We further confirm that the order of authors listed in the manuscript has been approved by all of us.

We confirm that we have given due consideration to the protection of intellectual property associated with this work and that there are no impediments to publication, including the timing of publication, with respect to intellectual property. In so doing we confirm that we have followed the regulations of our institutions concerning intellectual property.

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**Respectfully yours,**

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## **A Millifluidic-assisted ionic gelation technique for encapsulation of probiotics in double-layered polysaccharide structure**

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