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Functional neuroinflammatory- and serotonergic imaging in Alzheimer's disease

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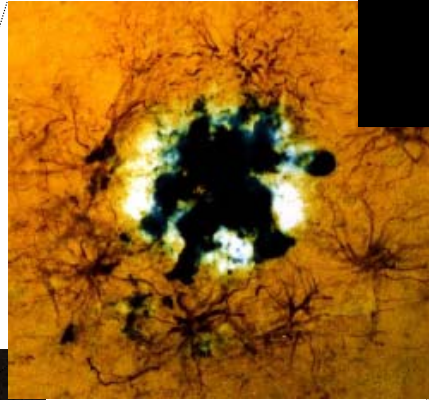
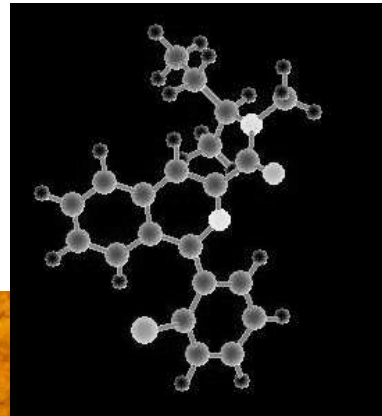
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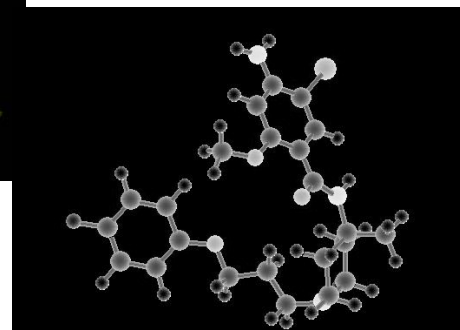
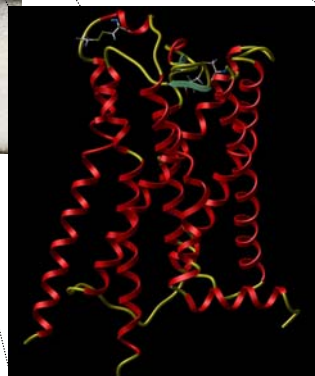
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Functional neuroinflammatory-
and serotonergic imaging in
Alzheimer's disease:
validation and preliminary
clinical findings



Josef Sudek (°1896 - †1976) was a famous Czechoslovakian photographer known for his lyrical images that show a fine eye for life's intimate details. He once explained that '*everything around us, dead or alive, in the eyes of a crazy photographer mysteriously takes on many variations, so that a seemingly dead object comes to life through light or by its surroundings... To capture some of this – I suppose that's lyricism*'. The cover photograph shows the work *Untitled* (1940) where *in the surrounding* of this PhD thesis one can depict *stoned* plaques and tangles.

The upper row represents the neuroinflammation part of this thesis where the first photograph shows an Alzheimer amyloid plaque (white) surrounded by reactive astrocytes (brown) and a cluster of microglial cells (black) sitting on top. Next to it, a three-dimensional model of the radioligand used in the present thesis PK11195 (either for PET or SPECT) is shown.

The lower row represents the serotonergic part of this thesis where the first picture shows a three-dimensional structure of the 5-HT_{2A} receptor. Next to it, a model of the SPECT radioligand R91150 is shown.

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Aan Sabine

RIJKSUNIVERSITEIT GRONINGEN

**Functional neuroinflammatory-
and serotonergic imaging
in Alzheimer's disease:
validation and preliminary clinical findings**

PROEFSCHRIFT

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aan de Rijksuniversiteit Groningen
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We must trust to nothing but facts. These are presented to us by Nature, and cannot deceive. We ought, in every instance, to submit our reasoning to the test of experiment, and never to search for truth but by the natural road of experiment and observation.

Antoine Lavoisier (1743-1794)

INTRODUCTION AND OUTLINE OF THE THESIS

The present thesis aims at clarifying the pathophysiology of Alzheimer's disease by means of functional radionuclide imaging, this in order to finally aid its therapeutic management. It is divided in two parts.

The *first part* deals with neuroinflammatory imaging in general with the ultimate goal of this part being the visualisation and assessment of neuroinflammatory lesions in Alzheimer's disease. Indeed, in the past decades, our understanding of the central nervous system has evolved from one of an immune-privileged site, to one where inflammation is pathognomonic for some of the most prevalent and tragic neurodegenerative diseases. Current research indicates that diseases as diverse as head trauma, multiple sclerosis, stroke and Alzheimer's disease exhibit inflammatory processes sharing this inflammatory pathway as a common mechanism contributing to cellular dysfunction and or neuron loss.

In **chapter two**, Alzheimer's disease as the most common form of dementia is thoroughly reviewed and an introduction is given on firstly Alzheimer's disease as an inflammatory disease and secondly neuroinflammatory imaging in general. In **chapter three**, an attempt is undertaken to visualise neuroinflammatory lesions in Alzheimer's disease with ^{57}Co and single photon emission computed tomography (SPECT), which has previously been proven useful in diseases like stroke and Multiple Sclerosis. To overcome the disadvantages encountered with the previous radioligand, a new radioligand (PK11195) was studied, which is described in **chapter four**. Since multiple sclerosis (MS) is the prototype neuroinflammatory disorder where inflammatory mediators contribute to white matter axonal damage leading to the accumulation of disability, radiolabelled PK11195 as a *neuroinflammatory marker* is validated in a cohort of MS patients. Therefore, its relationship with clinical measures on one hand and structural imaging on the other hand is assessed and described in **chapter five**. In **chapter six**, preliminary findings about radiolabelled PK11195 and its relationship with neuropsychological measures and perfusion imaging in a group of Alzheimer's disease patients are described.

The *second part* deals with the role and distribution of serotonin (5-HT) type 2A receptors in Alzheimer's disease (**chapter seven**).

In an *introductory part*, the role of serotonin in general and serotonin type 2A (5-HT_{2A}) receptors specifically in cognitive and non-cognitive behaviour and AD is briefly reviewed. In a *second part*, the distribution and comparison of the 5-HT_{2A} system using ^{123}I -5-I-R91150, a selective radio-iodinated 5-HT_{2A} receptor antagonist and SPECT in healthy controls and Alzheimer's disease is described together with its relationship with age, gender, concurrent depression and other neuropsychological measures.

CHAPTER TWO

INTRODUCTION TO NEUROINFLAMMATION, ALZHEIMER'S DISEASE AS AN INFLAMMATORY DISEASE, AND NEUROINFLAMMATORY IMAGING

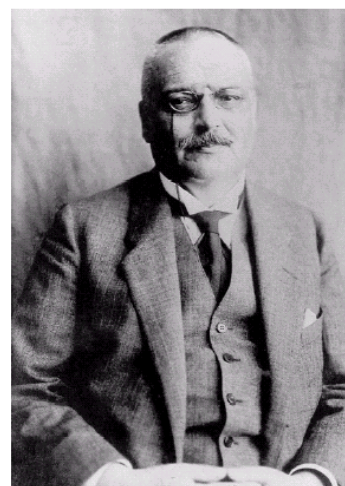
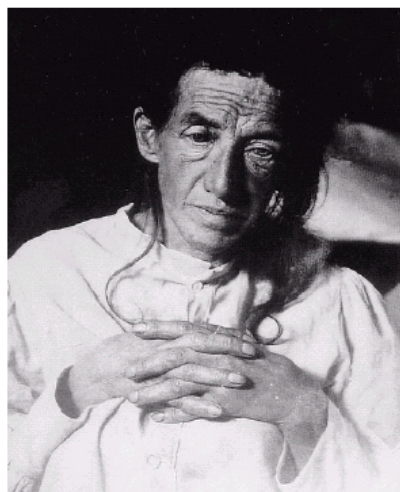
ALZHEIMER'S DISEASE

Depending on where you set your sights, Alzheimer's disease is a scientific puzzle, a medical whodunit, a psychosocial tragedy, a financial disaster or an ethical, legal and political dilemma. It is all those things and more – a complex problem that is a prototype for the health-care quandaries facing people in developed nations throughout the world. And the solution will need to be equally complex. The disease quietly loots the brain, nerve cell by nerve cell, like a burglar returning to the same house each night. As the brain loses mass, the rest of the body gradually shuts down...

Alzheimer's disease (AD) is the most common cause of dementia in the elderly and is a progressive neurodegenerative disorder that gradually robs the patient of his cognitive function and eventually causes death. The present part reviews the history, epidemiology, clinical features, pathophysiology, and treatment of AD.

HISTORY

Alzheimer's disease had played havoc with people since ancient times. Greek and Roman writers as well as Elizabethan chroniclers accurately described the symptoms of the illness. One of the best examples is in Shakespeare's King Lear. Lear is losing his memory and becoming disoriented; if you read between the lines, he has Alzheimer's disease. But Alzheimer's was not established as a distinct disease until the early part of this century. Alois Alzheimer (figure below, right) who later gave his name to this disease – in 1910 at the suggestion of Emil Kraepelin – first examined Auguste D, now considered as the first person described as having 'AD', in 1901 and followed her up until her death in 1906. After her death, he went on to study the neuropathologic features of her illness, in which he had a great interest due to his friendship with Franz Nissl, whose expertise helped with the development of the histological staining techniques essential in histopathology. Auguste D (figure below, left) was at the time of her first examination a 51-year old woman who initially presented with a strong feeling of jealousy towards her husband with carrying objects to and fro in her flat and hiding them. Later on, she showed progressive cognitive impairment, focal symptoms, hallucinations, delusions and psychosocial incompetence. Sometimes she felt that someone wanted to kill her and would scream loudly. After 4 ½ years of sickness, she died from septicaemia resulting from a decubitus ulcer in the sacral and left trochanteric regions. She presented the neurobiological changes found at necropsy – plaques, neurofibrillary tangles and atherosclerotic changes – now considered characteristic of AD [1]. In 1976 the neurologists Davies, Maloney, and Bowen showed that an enzyme necessary to synthesize acetylcholine was deficient in the brain of patients with AD. Earlier research in neurotransmitter chemistry had shown that cholinergic, or acetylcholine-containing, neurons play an important role in memory. The discovery of a link between a biochemical brain defect – the deficiency of acetylcholine – and AD marked the beginning of modern Alzheimer's research.



INCIDENCE, PREVALENCE, AND ECONOMIC IMPACT

AD accounts for 60 to 70% of the cases of progressive cognitive impairment in elderly patients. Prevalence of the disease in Europe ranges from 0.02% in people aged 30-39 years to 10.8% in those aged 80-90 years (more than 11 million people worldwide with lower incidence in people of African or Asian origin with even reports suggesting that AD does not occur in Nigerians) [2]. The prevalence of AD in the US doubles every 5 years after the age of 60 increasing from a prevalence of 1% among those 60- to 64-years-old to up to 40% of those aged 85 years and older [3]. The population of patients with AD will nearly quadruple in the next 50 years if the current trend continues [3]. The disease is more common among women than men by a ratio of 1.2 to 1.5 [4].

Most direct costs of care for patients with AD are absorbed by the expense of nursing home care, approximately 47 000,- € per patient per year [5].

Several risk factors for AD have been identified in epidemiologic studies in addition to age and female sex. The most potent risk factor is the presence of the apolipoprotein $\epsilon 4$ (APOE $\epsilon 4$) allele. Of its 3 forms $\epsilon 2$, $\epsilon 3$, and $\epsilon 4$ only the $\epsilon 4$ allele increases the likelihood of developing AD. The lifetime risk of AD for an individual without the $\epsilon 4$ allele is approximately 9% whereas the lifetime risk of AD for an individual carrying at least one $\epsilon 4$ allele is 29%. While representing a substantial risk of AD, the $\epsilon 4$ genotype is not sufficiently specific or sensitive for the diagnosis of AD to allow its use as a diagnostic test [6]. Other risk factors implicated in a variety of studies include head injury, low serum levels of folate and vitamin B12, elevated plasma and total homocysteine levels, family history of AD or dementia, fewer years of formal education, lower levels of fish in the diet, lower income, no daily wine consumption, lower occupational status, however other undisclosed genetic or environmental factors have yet to be determined [7, 8].

CLINICAL DIAGNOSIS

Although some sources report that AD can be diagnosed with over 90% accuracy during life if standard clinical criteria are followed, some available evidence suggests that mild dementia is rarely

diagnosed and even moderately severe dementia is underrecognized in clinical practice [9]. The specificity of the Mini-Mental State Examination is good (96%) but the sensitivity is poor (63%), indicating that by itself the test (using a standard cutoff score of 24) will leave a substantial proportion of cases of early dementia undetected. The typical clinical syndrome of AD includes three aspects. Firstly, deficits in cognitive functions which cause an amnesic type of memory defect with difficulty in learning and recalling new information, a progressive language disorder beginning with anomia and progressing to fluent aphasia, disturbances of visuospatial skills manifested by environmental disorientation and difficulties in copying figures, the inability to do motor tasks despite intact motor function (apraxia) and the inability to recognise, despite intact sensory functions (agnosia). There are usually deficits in executive function (planning, insight, judgment) and the patient is typically unaware of memory or cognitive compromise. All cognitive deficits progressively worsen. Secondly, neuropsychiatric and behavioural disturbances become apparent in AD, such as personality changes, delusions, hallucinations and misidentifications. Apathy is present early in the clinical course with diminished interest and reduced concern. Agitation becomes increasingly common as the illness advances and is a frequent precipitant of nursing home placement. Depressive symptoms are present in about 50% of patients and approximately 25% exhibit delusions. Thirdly, difficulties with activities of daily living manifest early in the disease, and affect functions such as handling money, use of the telephone, and driving (instrumental), and later, difficulties with dressing, feeding, and toileting (basic). Motor system abnormalities are absent in AD until the final few years of the disease; focal abnormalities, gait changes, or seizures occurring early in the clinical course of dementia make the diagnosis of AD unlikely. Patients with AD usually survive 7 to 10 years after onset of symptoms with a range of 2 to 20 years and typically die from bronchitis or pneumonia [10, 11]. Assessment and diagnosis of AD require identifying the core clinical features and excluding other common causes of dementia in the elderly. Screening for thyroid dysfunction and vitamin B12 deficiency is recommended; syphilis is no longer sufficiently common to warrant routine screening in typical clinical circumstances. Neuroimaging should be obtained to identify vascular contributions to the dementia syndrome and to identify other intracranial pathology. Functional imaging with positron emission tomography or single photon emission computed tomography are helpful particularly when clinical features are ambiguous [12].

PATHOLOGY

The current criteria for the pathologic diagnosis of AD require the presence of both senile neuritic plaques and neurofibrillary tangles in excess of the abundance anticipated for age-matched healthy controls [13]. Neuritic plaques consist of a central core of amyloid protein surrounded by astrocytes, microglia, and dystrophic neurites often containing paired helical filaments. Neurofibrillary tangles are the second major histopathological feature of AD. They contain paired helical filaments of abnormally phosphorylated tau protein that occupy the cell body and extend into the dendrites.

However, current evidence suggests that the neuropathology of AD comprises more than amyloid plaques and neurofibrillary tangles. At least a third of AD cases may exhibit significant

cerebrovascular pathology. Cerebral amyloid angiopathy, microvascular degeneration affecting the cerebral endothelium and smooth muscle cells, basal lamina alterations, hyalinosis and fibrosis are often evident in AD. These changes may be accompanied by perivascular denervation that is causal in the cognitive decline of AD. Peripheral vascular disease such as long-standing hypertension, atrial fibrillation, coronary or carotid artery disease and diabetes could further modify the cerebral circulation such that a sustained hypoperfusion or oligoemia is impacted upon the ageing brain.

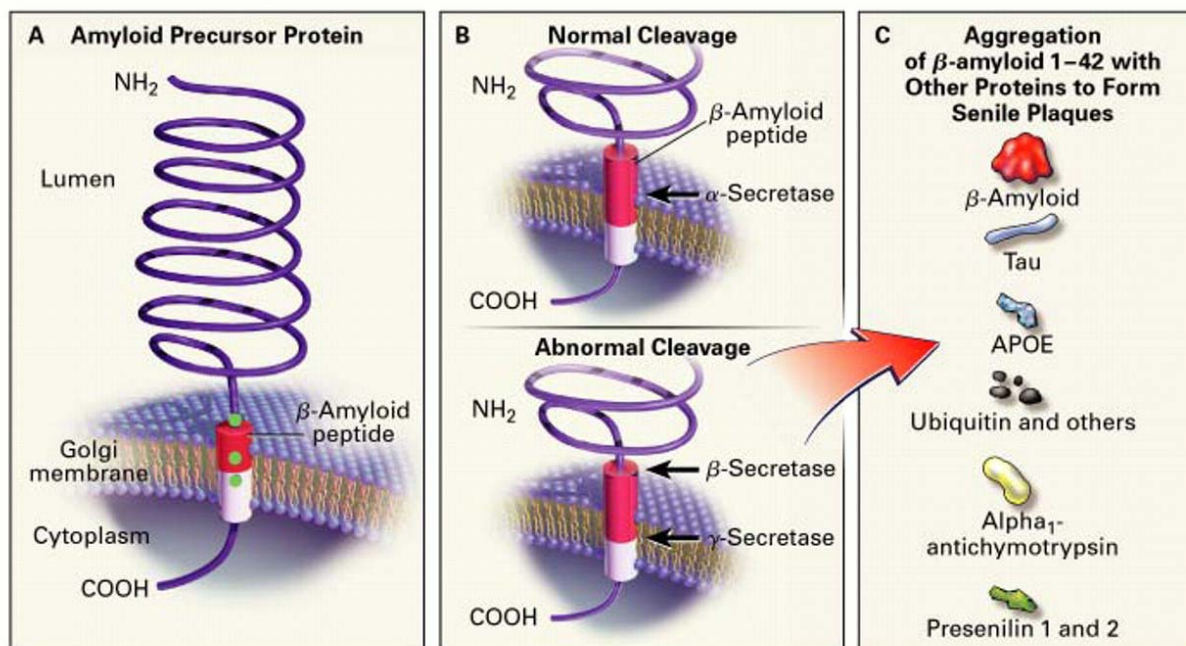
In addition to these three major classic histopathologic features, AD also is characterized by reductions in synaptic density, loss of neurons, and granulovacuolar degeneration in hippocampal neurons. Neuronal loss or atrophy in the nucleus basalis, locus ceruleus, and raphe nuclei of the brainstem leads to deficits in cholinergic, noradrenergic, and serotonergic transmitters, respectively with the cholinergic deficit as the most consistent neurochemical abnormality.

MOLECULAR GENETICS AND PATHOGENESIS

A small number of cases – between 2 and 7 percent – result from an inherited genetic mutation and can strike people as young as thirty. Although mutations account for so few cases of AD they have been of great value in the study of the pathogenesis of the disorder. Mutations in the amyloid precursor protein (APP gene, chromosome 21), presenilin 1 (chromosome 14), and the presenilin 2 gene (chromosome 1) produce an autosomal dominant pattern of inheritance with nearly complete penetrance [14]. Together with the apolipoprotein E gene, they account for about half the genetic risk.

The amyloid protein that appears to be central to the pathogenesis of AD is derived from APP (amyloid precursor protein) and its abnormal cleavage finally leads to the deposition of neuritic plaques (figure 2). The accumulation of β -amyloid initiates a series of events contributing to cell death, including activation of cell death programs, oxidation of lipids and disruption of cell membranes, an inflammatory response, and possible tangle formation, a close correlate of neuron loss. All of the identified mutations that cause AD result in increased production of β -amyloid protein [15].

Head injury, educational level, and other risk and protective factors identified through epidemiologic studies may exert effects on the likelihood of developing AD through their impact on cerebral reserve - the ability of the brain to withstand the accumulating amyloid burden without evidencing dysfunction and cognitive impairment [10].



TREATMENT

AD does not have a definite cure, but many psychosocial interventions and caregiver support can help to alleviate strain on carers. Available treatments for AD include cholinesterase inhibitors, disease-modifying treatments, and psychotropic agents. Treatment of AD must always reflect the values and wishes of the patient and their family. Therapeutic strategies may also change in the course of the disease, for example, slowing of disease progression with vitamin E may be desirable early in the clinical course but not in patients with advanced disease.

Cholinesterase inhibitors are the only medications approved by the US Food and Drug Administration as treatment for AD. Sufficient evidence has accumulated for these to be recommended as standard therapy for AD. Four inhibitors are currently available: tacrine, donepezil, rivastigmine, and galantamine. These agents have been shown to produce improvements in global function and cognition. Secondary benefits may include reduction in behavioral disturbances, temporary stabilization of activities of daily living, delay of nursing home placement, and reduced demands on caregiver time. Patients not responding to one agent in the class may respond to another. Discontinuation of treatment should be monitored; deterioration during withdrawal indicates therapeutic benefit and the medication should be reinstated [16].

Vitamin E and selegiline have been shown to reduce the rate of decline of functions in patients with AD. Evidence to support the use of other antioxidants, anti-inflammatory agents, or herbal medications such as ginkgo biloba is insufficient to recommend use as standard therapies. Estrogen in standard doses has been shown not to improve cognition in postmenopausal women with AD [16].

Reducing amyloid production, aggregation, or enhancing its removal are promising avenues of treatment that will address the basic pathophysiology of AD. Immunization, secretase inhibition, and other strategies to accomplish this are being studied.

Epidemiologic data suggest that nonsteroidal anti-inflammatory agents, hormonal treatments, histamine H2 blockers, antihypertensive agents, and statins may decrease the likelihood of developing AD [10, 17]. Clinical trials of these compounds to test their roles in the treatment or prevention of AD are planned or under way.

Psychotropic medications play a critical role in the management of behavioral disturbances of patients with AD. Relatively few psychotropic compounds have been tested specifically in AD populations. Recent double-blind, placebo-controlled trials have established the efficacy of the atypical antipsychotics risperidone and olanzapine for the treatment of psychosis and agitation in patients with AD [18]. Anticonvulsants such as carbamazepine also have been shown to have anti-agitation effects. Depression responds to treatment with selective serotonin reuptake inhibitors or tricyclic antidepressants; there are fewer adverse effects with the former.

Building an alliance with family caregivers is critical to success in the management of patients with AD. Family caregivers provide most of the care received by patients with AD over the course of their illness and are responsible for ensuring adherence to treatment regimens. Caregivers are prone to depression and physical illness as a result of the chronic stress associated with caregiving. Families benefit from short-term education programs and support groups [16].

CHALLENGES

Dramatic progress has been made in understanding the pathogenesis of and developing therapy for AD. Advances so far have had no impact on the prevalence of the disorder and have had limited effects on the clinical course. An effective response to the public health challenge presented by AD requires united efforts in drug discovery, clinical trials of promising agents, implementation in health care delivery systems of programs for screening and treatment of patients with AD, and governmental and public policy initiatives that support patients with AD and their caregivers in all stages of the disease. Much has been achieved but much more remains to be done to prevent the losses of cognitive function, emotional integrity, enjoyment of life, and personal dignity associated with AD. As such, the biggest question now is not whether our research will bear fruit, but how soon – for all those among us and all those to come who might otherwise be doomed to live in the plundered landscape of an eternal present.

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SCINTIGRAPHIC VISUALISATION OF INFLAMMATION IN NEURODEGENERATIVE DISORDERS

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SUMMARY

In the past decades, our understanding of the central nervous system has evolved from one of an immune-privileged site, to one where inflammation is pathognomonic for some of the most prevalent and tragic neurodegenerative diseases. Current research indicates that diseases as diverse as multiple sclerosis, stroke and Alzheimer's disease exhibit inflammatory processes that contribute to cellular dysfunction or loss.

Inflammation, whether in the brain or periphery, is almost always a secondary response to a primary pathogen. In head trauma, for example, the blow to the head is the primary event. What typically concerns the neurologist and neurosurgeon more, however, is the secondary inflammatory response that will ensue and likely cause more neuron loss than the initial injury.

The current paper reviews the basic neuroinflammatory mechanisms, the potential neurotoxic mediators during activation of microglia, the brain resident macrophages, and their role in neurodegeneration. To explore these mechanisms, Alzheimer's disease, with the expression of more than 40 inflammatory mediators the most extensively studied disorder in terms of immune-related pathogenesis, is taken as a *prototype*, also because of its importance as the most prevalent dementia type. Visualisation tools for these neuroinflammatory processes, both structural and mainly functional, are critically reviewed and discussed.

NEUROINFLAMMATION AND NEUROIMMUNOMODULATION

Introduction

"In vivo, veritas!" [1]

Current research has shown that the previous concept of the brain as an *immunologically privileged organ* is invalid. This notion was inferred from the lack of a lymphatic drainage system (now considered to be a lymph-like system [2]), its unusual tolerance to transplanted tissue, and the thought that lymphocytes were excluded from the central nervous system (CNS) by blood-brain and blood-cerebrospinal fluid barriers. As such, the immune and nervous system were considered different compartments acting autonomously in their contribution to physiological homeostasis [3].

One put a lymphocyte into a culture dish, added an antigen, and out came an antibody. So who needed a nervous system? However, already in 1891, Savchenko demonstrated that a CNS lesion could reverse a pigeon's nonsusceptibility to anthrax. Also, inflammatory episodes may be accompanied by behaviour or mood alterations, hypomotility and increased sleep, believed to assist the affected subject in fighting infections and prompting to confine to a safe shelter [1, 4]. Finally, a recent positron emission tomography (PET) study correlated immune measures and regional cerebral blood flow (rCBF). It was found that the natural killer cell activity correlated with rCBF in the secondary sensory cortex, whereas the proliferative lymphocyte response correlated with the rCBF in the secondary visual, motor, and sensory cortices, basal ganglia, and the left hippocampus, providing further support for the brain and immune system interaction [5].

Contemporary research learned that the blood-brain barrier (BBB) is, under certain conditions, less restrictive to the migration of monocytes, lymphocytes, or natural killer cells, irrespective of antigen specificity [6]. Moreover, *in vitro* and *in vivo* studies have clearly established that astrocytes and microglia (brain resident macrophages) can initiate an inflammatory cascade within the CNS [7]. Also, all components of the complement system are found in the brain and are produced by astrocytes, microglia, and, surprisingly, neurons.

However, several factors indicate that the CNS inflammation threshold is higher compared to the periphery, leading to a delay between peripheral and CNS inflammation during a general inflammatory status. For example, the rapid recruitment of neutrophils in the CNS is virtually absent, and monocytes are only recruited after a delay of several days. The reason for this higher threshold is at least threefold. Firstly, as only activated T-lymphocytes traverse the BBB, it is the small pool of peripherally activated T-cells that enter the CNS for immune surveillance [8]. Yet, without peripheral T-cell activation, antigens escape detection, thus, brain transplants survive, in spite of an antigen mismatch [9]. Secondly, there is an active suppression of antigen expression leading to T-lymphocytes not recognising their target neither activating inflammatory mechanisms [10]. Thirdly, the adhesion molecule expression, essential in cell-cell contacts during inflammatory cell migration, is low on cerebral endothelial cells [11]. Considered the above, it appears that the CNS, an organ exquisitely sensitive to inflammation, has evolved mechanisms to protect it from the potentially

damaging, even dramatic classical consequences of some acute inflammatory response aspects like redness, heat, swelling and pain, typically seen in the periphery.

Microglia

“Good, bad, or just ugly?” [12]

The concept of the presence of phagocytic brain cells was, although discovered by Nissl, studied in detail in the early part of the last century by Pio del Río-Hortega, a former student of the famous Spanish neuroanatomist Santiago Ramon y Cajal [13]. He identified a population of ramified cells, now considered to be resting microglia [14]. Although Jakob described their morphological changes into activated, macrophage-like cells in neurodegenerative disorders like neurosyphilis, rabies, Creutzfeldt-Jakob, senile dementia and Huntington disease already in 1927 [15], the origin and even the existence of this cell population was contested until recently. Few investigators followed up on these early pioneers during the next 50 years, largely because the staining method proved unreliable. This barrier came down only in the 1980's, after Perry at Oxford University began screening antibodies for their ability to bind microglia. It has only been during the last decade that major progress in microglial studies has been made, and their involvement in neurodegeneration has become apparent.

Microglia represent, next to astrocytes and oligodendroglia, 10-20% of the brain glial cell population (*glia* from Greek, meaning *glue*), located in close vicinity of grey matter neurons and between white matter fibre tracts. In contrast with the ramified shape along with a suppressed genomic activity in the *resting* state, on cellular activation, they assume an amoebic shape associated with a dynamic genome upregulation, characteristic of their phagocytic stage (Figure 1). They are the brain macrophages within the entire neuroaxis sharing the same lineage as monocytes, taking up residence in the CNS antenatally i.e. prior to the BBB completion. Cells of this lineage function as classical *professional* antigen presenting cells in the immune system in all mammals [16].

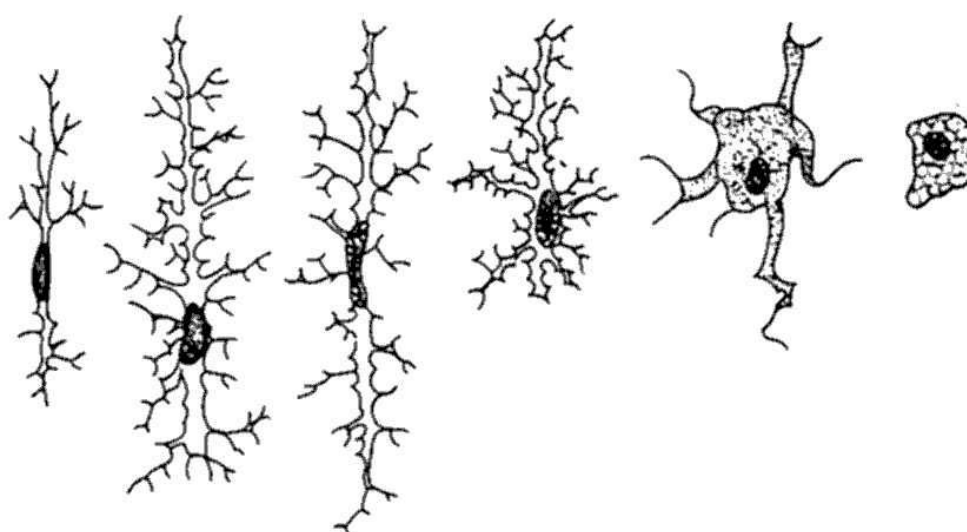


Figure 1. Morphology of ramified resting microglia with extended pseudopodia with transformation to the activated state with retraction of their branches (phagocytic cells or foamy macrophages, named *gitter cells* after Nissl in 1904 because of the fact they are typically *gitting* rid of dead myelin and other cell debris)

Microglia represent a highly reactive cell population and express antigens in response to microenvironmental stimuli, particularly neuronal damage. During the early neuronal injury stages, when affected brain tissue still appears histologically normal, microglia may carry out subtle microchanges such as the synapse removal from injured neurons. After non-lethal axotomy, for example, microglia interpose between pre- and postsynaptic moieties, cause synapse disconnection and strip the neuron of input (*synaptic stripping*). As such, they represent the primary immunocompetent cells dealing with invasions of any kind and removing cellular debris (i.e. scavenger cell, which may be important, combined with their ability to secrete growth factors, for tissue modelling in the developing CNS). All this, together with their ability to cooperate with immune cells, seems to make microglia function as true sentinels [17].

Conclusion

Immune cells, such as microglia, T-cells, or even neurons are able to produce potentially neurotoxic factors, some of them capable of destroying at picomolar concentrations. These factors, normally required for pathogen elimination, include cytokines, complement components, and reactive intermediates (superoxide anion, hydroxyl radicals, hydrogen peroxide, ...). These factors, however, not only destroy foreign pathogens but may damage local elements as well (*bystander lysis*), leading to neuronal loss [18]. Indeed, direct CNS injection of cytokines results in neurodegeneration, consistent with the potential role of cytokines in neurodegenerative diseases when microglia remain in an activated state and contrast with their potential neurotrophic actions under *transient exposure* or *housekeeping* conditions, where damaging actions are presumably *buffered* by cytoprotective mechanisms [19]. Also, microenvironmental compromises like age, genetic factors, and frank tissue insult will dramatically affect the neuron susceptibility as well as the *buffering capacity* degree for removing neurotoxic mediators. Moreover, there is little or no mitogenesis to repair potential damage. Concerning this postmitotic state, animal experiments already illustrated the neuronal vulnerability during inflammation, in particular of synaptic plasticity, memory, and neurotransmission [20]. Finally, in contrast to peripheral tissues, focal CNS injury not only has local effects, but also causes neuronal and axonal loss at a distance due to retrograde degeneration and Wallerian degeneration.

INFLAMMATION AND MICROGLIA IN CHRONIC NEURODEGENERATION, WITH THE EMPHASIS ON ALZHEIMER'S DISEASE

LINKING BRAIN IMMUNITY TO NEURODEGENERATION

"Good, bad, or irrelevant" [21]

As described above, CNS immune responses usually take milder courses, where it has not been clear yet whether this relative deficit is solely explicable by the lack of immunological structures, or due to counterregulatory mechanisms. Recent evidence indicates that CNS immune responses are indeed downregulated, with a key role for electrically active neurons. For instance, a blockade of neuronal activity in hippocampal cultures significantly increased the antigen expression on microglia [22].

Normally, CNS immune surveillance is effected by patrolling T-cells, freshly activated peripherally with an ensuing release of pro-inflammatory cytokines inducing glial cells to produce immunologically relevant molecules. Intriguingly, pro-inflammatory signals very similar to those provided by T-cells are also produced by degenerating brain cells. This pro-inflammatory milieu of neurodegeneration can be due to active induction signals communicated by degenerating neurons or cellular by-products of neurodegeneration (DNA, neurofilaments, and myelin fragments) [23], or, alternatively, it could reflect an escape from the anti-inflammatory control mentioned above [24].

Neurodegenerative diseases with immune system involvement are listed in Table 1.

CLINICAL CONDITION	FINDINGS (REFERENCES)
Diffuse Lewy Body disease	Microglia [25]
Progressive supranuclear palsy	Complement activation [26] Glial activation [27]
Corticobasal degeneration	Glial activation [27]
Parkinson's disease	Microglia [28] Complement activation [26] TNF- α [29]
Pick's dementia	(Micro)glial activation [27] Complement activation [30]
Huntington's disease	Microglia [31]
Creutzfeldt-Jakob disease	Microglia [32]
Multi system atrophy	Microglia [33]

Table 1. Neurodegenerative diseases (next to AD) associated with increased numbers of activated (micro)glia, increased CNS cytokines or complement activation

INFLAMMATION AS A CAUSE OF DAMAGE TO THE ALZHEIMER'S DISEASE BRAIN

Introduction

Alzheimer's disease (AD) is the most common form of dementia and the number of affected persons is expected to triple over the next 50 years. It is characterised by intraneuronal neurofibrillary tangles

(NFT), neuronal and synaptic loss, neurotransmitter deficits and amyloidosis. The latter results from the aggregation of β -amyloid peptides (i.e. $A\beta$, derived from the abnormal cleavage of amyloid precursor protein or β -APP), giving rise to amyloid or neuritic plaques [34].

Interestingly, when Alois Alzheimer in 1907 described its features, he also noticed a close association between brain phagocytes and amyloid plaques [35]. Nowadays, the pathophysiological relevance of inflammation to AD has been established by multiple lines of converging tangential and direct evidence. For example, transgenic animals (over)expressing inflammatory proteins exhibit neuropathological changes similar to AD,[36] whereas human beings without dementia but sufficient $A\beta$ /NFT to qualify for AD show only modest elevations of inflammatory markers [37].

The following sections briefly review the inflammatory mechanisms in AD.

Genetic risk factors and epidemiological data

AD shows an Apolipoprotein E (ApoE) genotype susceptibility with ApoE4 as a risk factor. Interestingly, ApoE4 seems essential for APP-induced microglial activation and the expression of several inflammatory indicators [38]. Also, several genetic cytokine risk factors have already been identified with a decreased cytokine activity associated with a reduced risk and delayed onset [39].

There are now about 20 reports which studied the AD incidence in populations with a long anti-inflammatory drug consumption history. Nearly all of these studies showed a lower AD incidence with a decrease of 50% or a delay in onset of 5 to 7 years, where, in one prospective study, the relative risk fell with increasing duration of drug use [40]. Clinical trials with indomethacin or propentofylline, another agent with anti-inflammatory properties, showed both a significant cognitive improvement [41, 42], while, however, one study with diclofenac and one recent study with hydroxychloroquine did not demonstrate a positive effect on AD progression [43, 44].

Immunopathological, in vitro, and in vivo data

A summary of these mechanisms is shown in Figure 2.

BACKGROUND

Just as foreign materials and damaged tissue are classical stimulants of peripheral, sometimes overtly cytotoxic, inflammation, so are also $A\beta$ and the ensuing neurodegeneration the most likely sources for inflammation in AD. From this point, a nearly bewildering number of inflammatory mediators comes in to play, each characterized by an abundance of amplifying and dampening loops, as well as multiple interactions with other subsystems. Like a web, all these inflammatory pathways make it likely for one set of mediators to induce most of the others. For this reason, the selection of any particular starting point for explaining the AD inflammatory mechanism must be taken as a matter of convenience [45].

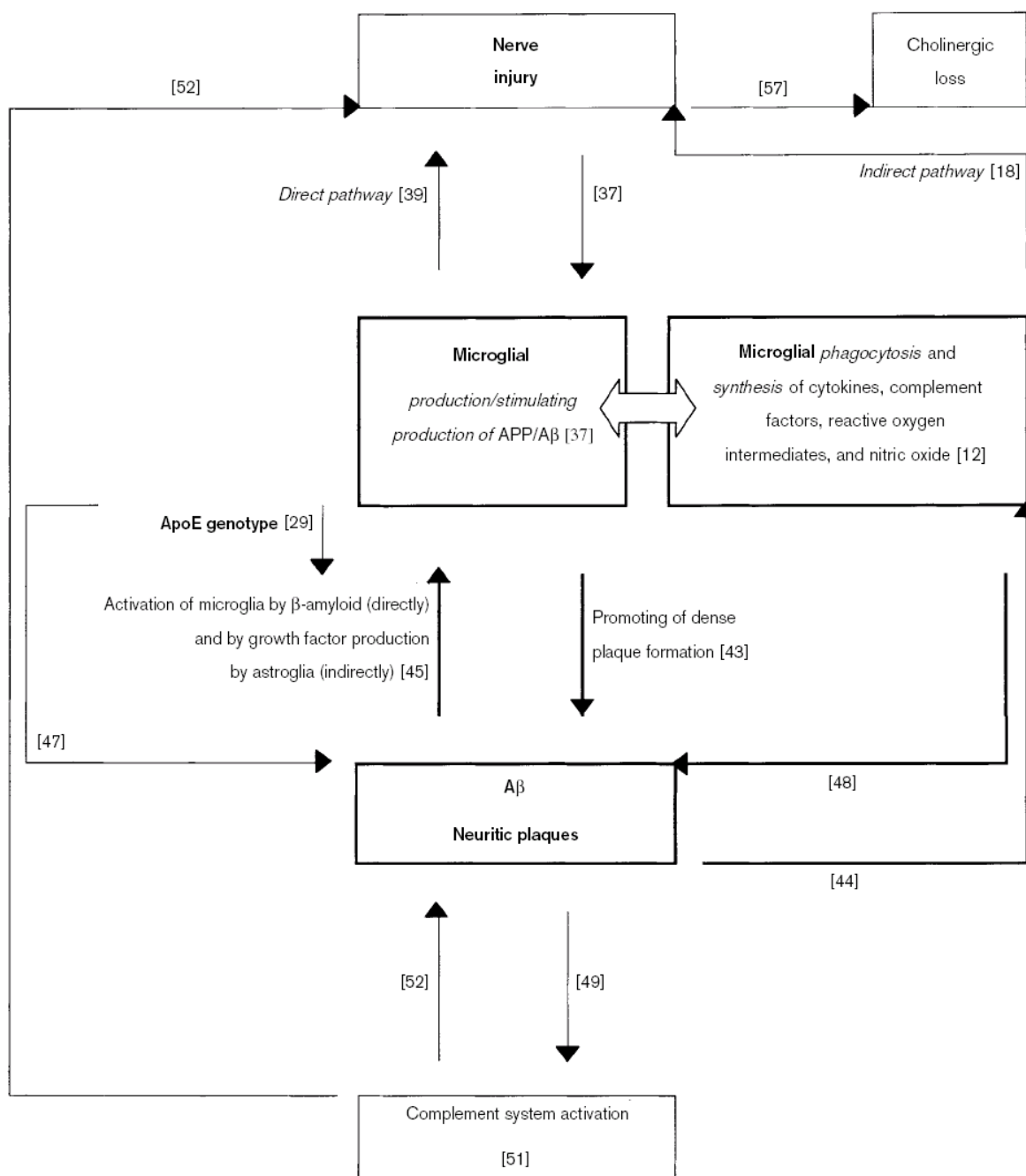


Figure 2. Inflammatory hypothesis in Alzheimer's disease emphasising the main loops with the interaction between microglia and the amyloid plaques and neurofibrillary tangles

SOURCES, TOXICITY, AND REMOVAL OF A β

The cellular source of A β is still a matter of debate. Microglia are able to synthesise A β in response to nerve injury or even A β itself [46]. As for toxicity, although it has been hypothesised that the presence of amyloid is the direct cause of AD pathology, the *in vivo* confirmation of A β toxicity has not yet been conclusively demonstrated, while there is even evidence that A β may be neuroprotective [47]. Moreover, in one study, a fulminant hippocampal neuron loss by neuritic plaques was only seen in the presence of microglia [48].

As for A β phagocytosis, the degradation rate seems limited and results in the release of potentially neurodestructive compounds [49]. However, that microglia can remove amyloid was strongly suggested by the demonstration of A β co-localised with microglia in *A β -immunised* transgenic mice, where amyloid was apparently cleared, where this removal also protected against a further cognitive decline [50]. Interestingly, C1q, a complement protein which binds A β , apparently inhibits the microglial A β uptake [51].

PLAQUE FORMATION AND MICROGLIAL INTERACTION THROUGH CYTOKINES AND COMPLEMENT SYSTEM

The fact that activated microglia are the sole and consistent accompaniment of neuritic plaques and not readily found in association with non-neuritic plaques suggests their pivotal role in the promotion of neuritic plaque formation, a role similar to that ascribed to peripheral macrophages in systemic amyloidosis [52].

A β may also act in a feedforward mechanism to maintain microglial activation, directly and indirectly by stimulating cytokine production, hereby increasing the amount of APP and rendering neurons subject to deleterious effects of activated microglia [53, 54].

Some cytokines cause neuronal injury and microglial activation with a further overexpression of the same cytokines, producing feedback amplification and self-propagation (*cytokine cycle*) [55]. Also, some cytokines who are on their own not neurotoxic are able to enhance the A β -induced cell death [56]. Finally, because APP/A β expression is regulated by the same transcriptional factors that are involved in the expression of most acute phase proteins, A β not only induces microglial cytokine release, but, once released, these same cytokines increase the A β aggregation process. The resulting vicious cycle could explain the chronicity of the disease [55, 57].

Recent studies suggested that A β and NFT bind C1q and activate the complement system in an antibody-independent fashion [58]. Also, both C5a and A β synergistically augment the release of proinflammatory cytokines. Moreover, the very modest upregulation of C1-inhibitor mRNA and the decrease of CD59 expression, both regulatory molecules protecting the cell from bystander while permitting foreign cell lysis, compared to the high upregulation for the other complement components, could lead to ongoing activation at the C1 level [59]. One study even indicated that complement production in the AD brain may be as great as in the liver, the primary source of complement [60]. This complement activation, of which direct evidence of its toxicity in the AD brain was recently observed, is also able to promote both A β aggregation and enhance the neurotoxicity of A β in neuronal cultures [61].

REGIONAL CELL LOSS AND COGNITIVE IMPAIRMENT

Cytokines affect acetylcholine, glutamate, and nitric oxide, all playing a key role in cognition [62]. Indeed, basal forebrain mixed neuronal/microglial cultures revealed cholinergic neuron losses, demonstrating their selective susceptibility to the toxic actions of activated microglia. More recently,

microglial secreted IL-1 was reported to induce the expression of the acetylcholinesterase protein and to increase its enzymatic activity [63]. Also, a disrupted memory-based performance in the water maze was shown after a sub-lethal bacterial injection while mice administered concurrently with IL-1 antibodies had normal learning rates [64]. Finally, IL-2 within the physiological range was capable of suppressing the hippocampal acetylcholine release, an effect related to the cognitive side effects during IL-2 immunotherapy in e.g. cancer patients [65]. Presumably, these data partly explain the cholinergic dysfunction in AD by demonstrating their susceptibility to toxic actions of activated microglia and suggest a basis for the regional loss of only selected neuronal populations in AD [66].

Remarks on the inflammatory hypothesis of AD

It should be stressed that the theory of inflammation as a primary disease-aggravating hallmark, opposed to a secondary or even a disease-ameliorating factor, remains a hypothesis and one should be aware that our current knowledge of microglia is still incomplete, speculative, and mainly based upon *in vitro* observations rather than *in vivo* studies [67]. Indeed, B- or T-cells and immunoglobulins are not readily detectable in the AD brain and are only in very small amounts found in relation to amyloid plaques (without IgM/IgA) [68]. Likewise, although leukocytes have been demonstrated, their role in AD has not been established [69]. As such, the evidence for an antigen-driven *acquired* immune response in AD, with T-cells eliminating amyloid and B-cells producing A β -specific antibodies, is not that overt as e.g. in multiple sclerosis (MS), although some authors see this *acquired immune response* inability as the support for the chronic overreaction of the *innate immune system* (phagocytic cells) [70].

NEUROINFLAMMATORY IMAGING

INTRODUCTION

Visualising neuroinflammation would be of interest, firstly for clarifying the pathophysiology, secondly for selecting patient subgroups that are more eligible for anti-inflammatory treatment and finally, for monitoring patients during trials with these anti-inflammatory agents. In the following section the currently available neuroinflammatory imaging modalities, both structural and mainly functional, will be reviewed and discussed.

STRUCTURAL IMAGING

As its name implies, the capability of structural imaging lies in visualising its (non-specific) structural changes and describing the detailed spatial relationship of inflammatory consequences like mass effects, oedema, vascular congestion, thrombosis, petechial haemorrhages, secondary demyelination, gliosis, and finally neuronal destruction, necrosis, or atrophy. As such, computed tomography (CT) and to a greater extent (Gadolinium-enhanced) magnetic resonance imaging (MRI), with its excellent soft tissue contrast resolution (mainly for evaluation of white matter and posterior fossa) are able to detect CNS inflammatory changes caused by mostly localised processes like cerebral abscess, encephalitis, granulomatous disease (tuberculosis, sarcoidosis, ...), meningitis, empyema, AIDS, chronic inflammatory demyelinating polyneuropathy, and MS [71]. For example, Brück *et al.* found that demyelinating lesions in MS, presenting as isointense lesions with a massive gadolinium-DTPA enhancement on T1-weighted scans, correlated neuropathologically with activated macrophages in the zone of myelin destruction at the plaque border [72].

However, in general, inflammation must be already at an advanced stage before it can be depicted by one of these imaging modalities, giving rise to its poor sensitivity at the early stages of inflammation (when anatomical changes are not detectable yet). Also, for chronic processes, structural changes may be detectable that do not reflect the actual state of disease activity. Indeed, Ketonen *et al.* noted already that in early AIDS dementia encephalitis, post-mortem characterised by scattered microglial nodules and HIV-infected multinucleated giant cells located primarily in the white matter and correlating with the severity of dementia, both CT and MRI are insensitive enough to detect these microglial nodules and for this reason, the neuroimaging appearance early in the disease is usually normal [73]. Similarly, Kim *et al.* noted that, although CT and MRI are able to detect general or basal ganglia atrophy and white matter lesions that appear to increase in severity with the progression of the HIV infection, these techniques are relatively insensitive to the presence of clinical dementia, neurological signs, or positive findings on neuropsychological tests. In addition, they show poor correlation with histopathological findings [74].

METABOLIC IMAGING

As for the newer structural or *metabolic* imaging tools in brain inflammation, Cecil *et al.* reviewed proton MR spectroscopy as a sensitive and specific imaging tool in Creutzfeldt-Jakob, herpes simplex encephalitis, and AIDS, indicating its applicability for longitudinal studies to predict and monitor the

response to therapy, leading to an individual optimised treatment [75]. Likewise, Bitsch *et al.* found that the measured increases of choline and myo-inositol corresponded to the histopathologically verified glial proliferation and the infiltration of subcortical grey matter structures with foamy macrophages [76]. Recently, Rovaris *et al.* reported about the value of magnetisation transfer imaging (MTI) in measuring brain involvement in systemic immune mediated diseases. It was found that MTI provides information about brain damage with increased pathological specificity and detects subtle microscopic abnormalities in the normal brain tissue, which go undetected with conventional scanning. However, in some immune mediated diseases microscopic brain tissue damage seemed to be absent despite macroscopic MRI lesions or clinical evidence of CNS involvement [77].

FUNCTIONAL RADIONUCLIDE IMAGING

Background

Nuclear medicine provides several techniques for the detection of inflammation. Studies demonstrating inflammatory lesions started as early as in 1959, when Athens *et al.* labelled leukocytes by intravenous injection of diisopropylfluoro-phosphate labelled with ^{32}P with which they demonstrated skin blisters in volunteers [78]. Classically, scintigraphic imaging of inflammation has been done with ^{67}Ga -citrate, radiolabelled leukocytes, nanocolloids, non-specific human immunoglobulins (HIG), and ^{18}F -deoxyglucose (FDG). Their uptake mechanism ranges from direct binding to relevant inflammatory cells or proteins (radiolabelled leukocytes, ^{67}Ga -citrate, HIG) over hyperaemia, binding to lactoferrin excreted *in loco* by leukocytes or to siderophores produced by micro-organisms (^{67}Ga -citrate), non-specific locally increased blood supply, extravasation through vessels with increased vascular permeability giving rise to an expanded local interstitial fluid space (^{67}Ga -citrate, nanocolloid, HIG), to high glucose uptake in inflammatory cells (FDG) [79]. As such, studies with radiolabelled leukocytes in cerebral ischemia have been undertaken where several authors reported on the higher accumulation in massive infarcts with severe neurological impairments and little improvement [80]. As far as chronic mononuclear cell infiltrates are concerned, however, most radiopharmaceuticals show inadequate diagnostic accuracy [81]. This is due to the minor haemodynamic and permeability changes (little or no vasodilatation), the slow cellular turnover and the predominant mononuclear cell infiltrate of chronic processes.

In the last decade, attempts have also been made to visualise inflammation by means of Cobalt radioisotopes. Indeed, both *in vivo* and *in vitro* experiments have shown that Ca^{2+} accumulates in the (ir)reversibly damaged nerve cell body and degenerating axons [82, 83]. Cobalt radioisotopes, as Ca^{2+} -analogues, probably reflect Ca^{2+} -influx in ischaemically or neurotoxically damaged cerebral tissue. Moreover, the time sequence of the radioligand uptake seems to correlate with cell death and glial proliferation in the ipsilateral thalamus following supratentorial ischaemic stroke in an experimental rat stroke model [84]. In this way, both ^{57}Co (for single photon emission tomography or SPET) and ^{55}Co (for PET) were able to visualise some of the focal neurodegenerative changes, reactive gliosis, endangered brain tissue and/or ongoing neuronal tissue decay including inflammatory lesions in various brain diseases e.g. multiple sclerosis, trauma, tumours, and stroke [80, 85, 86]. A

recent study however, concluded that ^{57}Co SPET was not able to show any regional raised uptake in AD patients, irrespective of the depth or extent of the associate perfusion defects, the presence of atrophy on MRI, or the neuropsychological test results [87]. Moreover, the long physical half-life with its resulting low count rate and statistics and the incomplete knowledge about the specific cellular uptake mechanisms all limit the application of Cobalt radioisotopes.

Radiolabelled receptor-specific proteins and peptides

Over the last decade, there has been a shift in scintigraphic inflammatory imaging from large proteins with non-specific uptake mechanisms via receptor-specific large proteins to receptor-specific small proteins and peptides (i.e. mediators of the inflammatory response), allowing the non-invasive detection of specific cells and tissues [88]. Monoclonal antibodies (against leukocyte antigens or endothelial adhesion molecules) were the first example of this new class of radiopharmaceuticals and in the past few years several new radiolabelled receptor ligands have been developed. As such, radiolabelled monoclonal antibodies against granulocyte and lymphocyte antigens, adhesion molecules, cytokines, chemokines, chemotactic peptides, and macrophages were developed [81]. For example, Paul *et al.* recently reported the detection and quantitation of neuroinflammation through BBB permeability changes during experimental allergic encephalomyelitis using a radiolabelled tuftsin analogue [89]. Tuftsin is a tetrapeptide derived from the Fc portion of IgG that promotes chemotaxis and phagocytosis of neutrophils, monocytes, and macrophages by binding to receptors on these cells. In addition, the radiopharmaceutical was able to successfully monitor glucocorticoid suppression of inflammation, recording a typical dose-response to increasing steroid concentrations.

All of these mediators came available for application in several fields by synthesis or recombinant DNA techniques. In nuclear medicine, they have emerged as a promising class of agents with attractive characteristics for scintigraphic detection of inflammation. Theoretically, the high binding affinity for their receptors – expressed in inflammatory tissue – facilitates retention of these agents in inflammation while the small size permits rapid clearance from blood and other non-target tissues. Whether this small radiolabelled receptor-binding agent specifically localises in an inflammatory focus depends firstly on the receptor expression in the particular inflammatory response. Secondly, the receptors should be accessible for the ligand and thirdly, the interaction of the ligand and its receptor should be characterized by high affinity and specificity (shown by autoradiography, receptor blockade, or studies with control agents). For neuroimaging studies in pathologies without BBB breakdown, the ligand should also easily penetrate the BBB.

Toxicity is still the major drawback of using receptor-specific small proteins and peptides for scintigraphic imaging. The tested agents are mediators of the inflammatory response and most of them elicit a specific response after binding to the receptor, i.e. express biological agonistic activity, which is undesirable for scintigraphic imaging. The use of receptor antagonists is therefore a logical choice, however, antagonists behave differently from agonists. Alternatives are the development of

partial antagonists with significantly reduced biological activity, obtained by synthesis or modification of the agonists, or the development of high specific activity labelling of agonists [90].

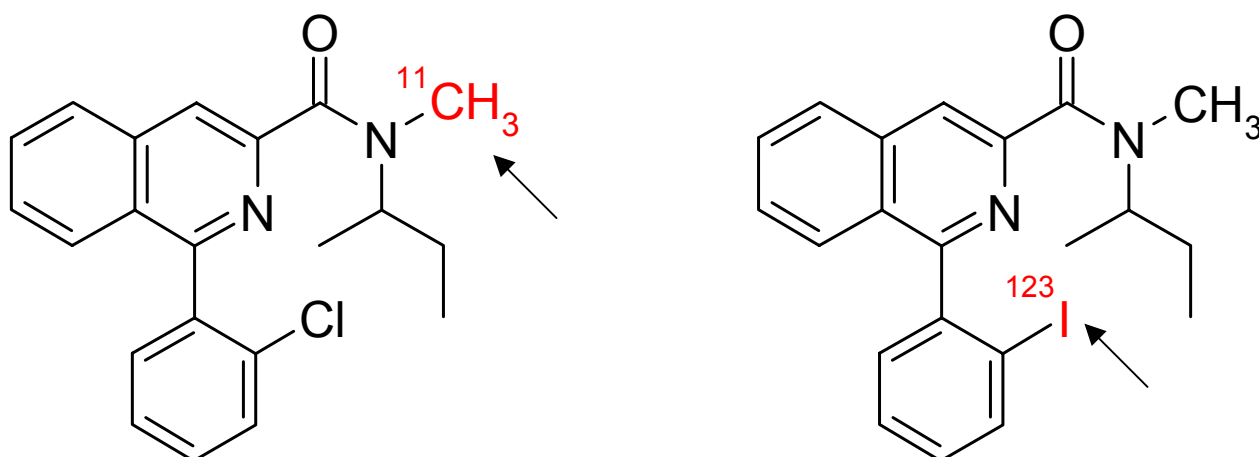


Figure 3. Chemical structure of PK11195 (the arrows indicate the site for radiolabelling with ^{123}I (SPET, right) or ^{11}C (PET, left))

Imaging of Microglia

The scintigraphic visualisation of microglia can be performed with radiolabelled PK11195, a ligand that binds the peripheral benzodiazepine receptor (PBR), present on microglia and upregulated under inflammatory circumstances. The PBR is structurally and pharmacologically distinct from the central benzodiazepine receptor (associated with GABA-regulated chloride-channels), and earned his name based on its localisation outside the CNS and its high affinity for several 1,4-benzodiazepines. The PBR is found in highest concentrations in kidneys, colon membranes, heart, steroid hormone producing cells of adrenal cortex, ovaries and testes, and several cell types of the immune system, such as mast cells and macrophages. It is also present in low concentrations throughout the brain, primarily associated with the choroid plexus, ependymal linings, and glial cells [91].

Although the specific function of the PBR remains unknown, it is generally accepted to be involved in lipid metabolism and/or transport, heme biosynthesis, cell proliferation, or ion channel functions [91]. Its immunomodulatory role includes the ability to induce monocyte chemotaxis, modulate cytokine expression and superoxide generation, and stimulate antibody-producing cell formation [92]. Interestingly, the PBR has the ability to reflect neuronal injury and neurotoxicity, by a rise in the number of binding sites in the case of activated microglia [93, 94].

PK11195 (1-(2-chlorophenyl)-N-(1-methyl-propyl)-3-isoquinoline carboxamide) is a specific and selective high affinity ligand for the PBR and, in this way, can be used as a marker for neuroinflammatory lesions (Figure 3). It has neither anxiolytic nor spasmolytic activity, nor interactions with other receptors and has been classified as an antagonist or partial agonist [95]. As such, Banati

et al. showed an increased PK11195 binding to activated microglia after facial nerve axotomy - a lesion causing a retrograde neuronal reaction without nerve cell death with a rapid proliferation and activation of microglia while keeping the BBB intact - where the peak of PK11195 binding was observed 4 days after the peripheral nerve lesion, which is consistent with the well-known time course of microglial activation. Moreover, photoemulsion microautoradiography confirmed the restriction of PK11195 binding to activated (i.e. PBR-expressing) microglia, where the full transformation of microglia into parenchymal phagocytes is not necessary to reach maximal levels of PK11195 binding. It was concluded that PK11195 is a well-suited marker of microglial activation in areas of subtle brain pathology, without BBB disturbance, or the presence of macrophages [96].

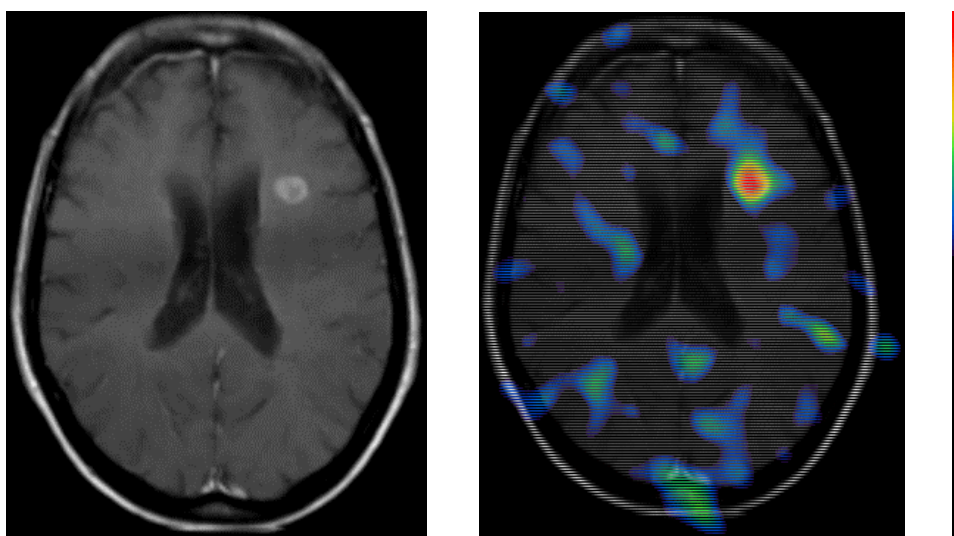


Figure 4. Transaxial slice of an MRI of an MS patient showing gadolinium-enhancement on a T1-weighted scan (left) and overlaid MRI- ^{11}C PK11195 PET image showing the focus of radioligand uptake at the same site (right)

In vivo visualisation of the human PBR, and in this way of neuronal damage, cellular inflammatory infiltration, or microgliosis, has previously been done with ^{11}C radiolabelled PK11195 for PET in various diseases like glial neoplasms, ischemic stroke, MS, Rasmussen's encephalitis, AD and Parkinson's disease, producing a signal of activated microglia unrelated to the influx of blood-borne macrophages (Figure 4) [97-100]. Also, significant ^{11}C -PK11195 binding was detected in MS patients in areas where MRI did not show any abnormalities, e.g. PK11195-related signals localised to deafferented grey matter regions such as the lateral geniculate body (to which the optic nerve projects) and visual cortex in patients with previous optic neuritis. In patients with transient speech dyspraxia, regionally increased PK11195 binding was found in the left frontal operculum close to Broca's area, which contains the superior longitudinal fascicle [101]. Finally, ^{11}C -PK11195 has also been applied in early and mild dementia patients revealing an increased regional binding in the entorhinal, temporoparietal, and cingulate cortex. Moreover, serial volumetric MRI scans revealed that areas with high ^{11}C -PK11195 binding subsequently showed the highest rate of atrophy up to 12-24 months later indicating that the presence of a local immune response in cortical areas did indeed reflect an active disease process associated with tissue loss. Also, measurement of cerebral glucose

metabolism revealed that areas with high ^{11}C -PK11195 binding were also characterised by decreased regional glucose use. Finally, in one patient with isolated memory impairment without dementia, the pattern of atrophy as seen by volumetric MRI imaging was predicted by the initial distribution of increased ^{11}C -PK11195 binding [102].

Recently, the biodistribution and dosimetry of PK11195 radiolabelled with Iodine for SPET has been studied. It was concluded that ^{123}I labelled iodo-PK 11195 is a suitable agent for the visualisation of the PBR and indirectly for the imaging of neuroinflammatory lesions [103]. In a recent pilot study, [^{123}I]iodo-PK 11195 was also applied in AD which showed a distinct difference in ligand uptake between AD patients and controls, indicating the pathophysiological involvement of microglia, in frontal, temporal and parietal cortical regions, pathognomonically compromised in AD [103]. Moreover, inverse correlations were found between regional [^{123}I]iodo-PK11195 uptake values and cognitive test results. In this way, the radioligand PK11195, developed both for SPET and PET, can be considered as a highly sensitive cellular marker for the functional monitoring of microglia *in vivo*, useful for the visualisation of chronic neurodegeneration without BBB breakdown nor other imaging findings.

CONCLUSION

In this review, the current status of inflammation with respect to neurodegeneration has been highlighted. From the basic neuroinflammatory mechanisms and its biochemical characteristics, the role of its potential mediators playing a key role in neurodegenerative disorders has been explored, with Alzheimer's disease as a prototype. Currently, the overwhelming amount of *in vitro* data has to be translated to *in vivo* human data. Whereas structural imaging shows merely late anatomical consequences of an inflammatory response, functional imaging is a strong potential candidate to bridge this gap between *in vitro* and *in vivo* knowledge. A number of radioligands have been recently explored which allow the early *in vivo* visualisation of inflammatory responses, and, as such, open a promising window on both *understanding* as well as possible *clinical management* of inflammatory neurodegenerative disorders.

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CHAPTER THREE

COBALT AS AN INFLAMMATORY TRACER IN ALZHEIMER'S DISEASE

**⁵⁷Co SPECT, ^{99m}Tc-ECD SPECT, MRI, AND NEUROPSYCHOLOGICAL TESTING IN
SENILE DEMENTIA OF THE ALZHEIMER TYPE**

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SUMMARY

Introduction: Inflammatory mechanisms contribute to the pathophysiology in senile dementia of the Alzheimer type (sDAT). Previous studies showed that ⁵⁷Co SPECT is able to visualise inflammatory lesions, probably by means of the final common pathway of the Ca²⁺-homeostasis disturbance in both neuronal degeneration and inflammation. The aim of this study was (1) to detect ⁵⁷Co SPECT changes in sDAT patients, (2) correlate these findings with conventional neuroimaging techniques and neuropsychological testing (NPT), and (3) compare ⁵⁷Co SPECT findings in sDAT patients with other types of dementia.

Patients and methods: Six patients suffering from probable sDAT were included and compared with 4 patients suffering from other types of dementia. All patients had a MRI-scan, NPT, ⁵⁷Co and a ^{99m}Tc-ECD SPECT scan. Perfusion SPECT images were semiquantitatively evaluated by comparison with an age-matched normal database while ⁵⁷Co SPECT scans were assessed qualitatively.

Results and conclusions: MRI and ^{99m}Tc-ECD SPECT scans yielded conclusive results as to the exclusion of other pathologies and confirmation of diagnosis. Using visual analysis, ⁵⁷Co SPECT scans were not able to show any regional raised uptake, irrespective of the disorder, depth or extent of the perfusion defects, presence of atrophy on MRI, or the results of NPT.

INTRODUCTION

In most industrialised countries, senile dementia of the Alzheimer type (sDAT), a primary degenerative disease of the brain, either alone or in combination with other illnesses, accounts for about 70% of dementia cases. The typical course in sDAT is one of progressive decline with an average survival of 8 to 10 years. The most characteristic feature is progressive memory impairment, predominantly loss of short-term memory. However, other cognitive dysfunctions or behavioral symptoms, as well as changes in the neurological status (especially late sDAT) are important [1].

Pathophysiologically, sDAT is characterised by dense and neuritic amyloid plaques, cerebral intraneuronal neurofibrillary tangles (NFT), neuronal and synaptic loss and deficits in neurotransmitter functions [2]. However, over the last years, it has become clear that inflammatory mechanisms may contribute to the neurodegenerative process in sDAT. Indeed, epidemiological data from about 20 studies have shown the protective and progression-retarding effect of non-steroidal anti-inflammatory drugs (NSAIDs) which would reduce the prevalence by 50% of sDAT in people who regularly take these drugs for various reasons [3]. As such, Breitner et al. concluded from twin studies that the use of NSAIDs could delay the onset of sDAT by 5 to 7 years [4]. As for treatment, there is only one double-blind placebo-controlled clinical trial showing this same progression-retarding effect [5].

Visualising this inflammation with positron emission tomography (PET) or single photon emission computed tomography (SPECT) would be of interest, firstly for clarifying the underlying pathophysiology, secondly for selecting subgroups of patients that are more eligible for anti-inflammatory treatment and finally, for monitoring patients during trials with anti-inflammatory agents.

Both *in vivo* and *in vitro* experiments have shown that Ca^{2+} accumulates in the (ir)reversibly damaged nerve cell body and degenerating axons, this through a passive influx due to a shortage of ATP following ischemia, resulting in the disappearance of the membrane potential, and through neuronal and glial uptake by divalent cation-permeable kainate-activated non-NMDA glutamate receptor-operated channels in the membrane [6-11]. ^{57}Co (SPECT) and ^{55}Co (PET), both as Ca^{2+} -analogues, reflect Ca^{2+} -influx in ischaemically or neurotoxically damaged cerebral tissue. In this way, both ^{57}Co SPECT and ^{55}Co PET have been shown capable of visualising focal neurodegenerative changes, reactive gliosis, endangered brain tissue and/or ongoing neuronal tissue decay including inflammatory lesions in various brain diseases e.g. multiple sclerosis, trauma, tumours, and stroke [12-18]. Moreover, the time sequence of the ^{55}Co -load seems to correlate well with cell death and glial proliferation in the ipsilateral thalamus following supratentorial ischaemic stroke in an experimental rat stroke model [19]. The visualisation of these inflammatory processes in sDAT can be expected to occur by means of the final common pathway of the Ca^{2+} -homeostasis-disturbance in both neuronal degeneration and inflammation [20-24].

A previous study by Oosterink et al. with PET and ^{55}Co suggested that this technique could generate additional specific information, which cannot be obtained with conventional neuroimaging techniques

like perfusion and ^{18}F FDG PET [25]. The objectives of this study were (1) to visualise inflammation *in vivo* in sDAT patients by detecting ^{57}Co SPECT changes and investigate whether ^{57}Co SPECT can generate additional information which cannot be obtained with conventional neuroimaging techniques or neuropsychological testing (NPT); (2) to search for a possible correlation of findings with data obtained from MRI, perfusion SPECT, and NPT; and (3) to compare findings in sDAT patients with patients suffering from vascular dementia (VaD) and frontal lobe-type dementia (FLD).

PATIENTS AND METHODS

PATIENTS

The study was approved by the medical ethics committee and all patients gave informed (proxy-)consent. Six patients suffering from probable sDAT (mean age 79 ± 7 yrs; range 68 to 87 yrs) according to the NINCDS-ADRDA criteria were included [26]. As controls, 3 VaD patients (mean age 67 ± 5 yrs) according to the NINDS-AIREN criteria and one FLD patient (75 yrs) according to the criteria suggested by Gustafson et al. were included [27, 28].

METHODS

Magnetic Resonance Imaging

All patients had a MRI scan (1,5 Tesla, Siemens, Erlangen, Germany). After the administration of Gadolinium, 5 mm axial slices were scanned with protondensity-, T_2 - and T_1 -weighting. Subsequently, the head was scanned with a 3D-MPRAGE sequence yielding 128 sagittal T_1 -weighted images with a thickness of 1.25 mm. From the MPRAGE series, axial, sagittal, and coronal planes were reconstructed. The images were hard copied and then viewed to assess global/regional atrophy, white matter lesions (periventricular, frontoparietal, occipital, and temporal), and the presence of infarcts.

Neuropsychological testing

Patients underwent the following battery: mini mental state examination (MMSE; N=10), Rey auditory verbal learning test for verbal learning and memory (AVLT; N=9), Trail making test for attention, sequencing, mental flexibility, and visual search and motor function (TMT, N=7), Controlled Oral Word Association Task for semantic and syntactic verbal fluency (COWAT, N=8), and the Money Road map test for spatial orientation (MRMT, N=8). Not all tests could be performed in every patient due to non-compliance.

^{57}Co SPECT scan

^{57}Co was purchased from Amersham (Amersham Cygne, Eindhoven, the Netherlands). Approximately 37 MBq (1 mCi) of ^{57}Co was injected. The patient was scanned on a triple-headed gamma camera (Toshiba GCA-9300A, Dutoit Medical, Wijnegem, Belgium) equipped with low energy, high-resolution parallel hole collimators (FWHM 9.5 mm), 15 ± 10 hours (range 3 to 24) after injection, in the same session as the $^{99\text{m}}\text{Tc}$ -ECD SPECT scan, enabling image registration. Images were acquired in a 128×128 matrix with a step angle of 6, frame time of 90 seconds, and a 1.25 zoom. Images were reconstructed with filtered backprojection (FBP, Butterworth filter 0.9 cycles/cm, order 8). Uniform attenuation correction was performed ($\mu=0.09$), no scatter correction was applied. A visual qualitative assessment of the ^{57}Co SPECT images was made.

$^{99\text{m}}\text{Tc}$ -ECD SPECT scan

Nine patients underwent a $^{99\text{m}}\text{Tc}$ -ECD SPECT scan, after the injection of 925 MBq $^{99\text{m}}\text{Tc}$ -ECD (ethyl cysteinat dimer; Dupont Pharmaceuticals Ltd., Belgium). Images were acquired in a 128×128 matrix with a frame time of 60 seconds, a step angle of 6, and a 1.25 zoom. Images were reconstructed with FBP (Butterworth filter 0.9 cycles/cm, order 8). Uniform attenuation correction was performed ($\mu=0.09$), without scatter correction. Perfusion SPECT images were automatically fitted and realigned into Talaraich co-ordinates where 26 cortical, 6 subcortical, 2 cerebellar, and one pons 3D-volumes of interest were assessed semiquantitatively (normalisation total number of counts) (Brass software, Nuclear Diagnostics, Sweden). Comparison was done to a database consisting of 20 healthy controls (mean age 70.4 ± 6.2 yrs) [29]. Mean counts per voxel were averaged in the sDAT group to assess a group perfusion deficit. A hypoperfusion in a specific region was considered as

significant when the uptake was less than the averaged uptake for the healthy volunteers minus two times the SD for that specific region.

RESULTS

Age, pathology, MMSE-score, the presence of cerebral infarcts on MRI and the perfusion defects are presented in Table 1. Age was inversely correlated with the relative perfusion in the left temporal lobe, temporal atrophy, the MMSE-score and the number of hyperperfused regions ($p = 0.04$, Pearson correlation; $p = 0.01$, $p = 0.02$, and $p = 0.02$, Spearman correlation coefficient) respectively.

Age	Pathology	MMSE	Infarcts on MRI	Significant perfusion defects
75	sDAT	12	(-)	L and R temporal superior, medial inferior, and parietal inferior region
68	sDAT	19	(-)	L prefrontal and superior frontal region; posterior cingulate gyrus
84	sDAT	16	(+)	L temporal superior and parietal inferior region; cerebellum
83	sDAT	0	(-)	L temporal superior region
87	sDAT	10	(-)	L lateral frontal, temporal medial inferior, and parietal inferior region R lateral frontal and temporal anterior region
77	sDAT	22	(-)	R prefrontal region and posterior cingulate gyrus; thalamus
68	VaD	17	(+)	Not performed
71	VaD	18	(+)	R lateral/superior frontal, temporal medial inferior, and parietal superior region
61	VaD	24	(+)	R temporal anterior region, cerebellum
75	FLD	17	(-)	L lateral frontal and R prefrontal region

sDAT = senile dementia of the Alzheimer type; VaD = vascular dementia; FLD = frontal lobe-type dementia

Table 1: Age, pathology, MMSE-score, presence of infarcts on MRI and the significant perfusion defects detected on the ^{99m}Tc -ECD SPECT scans

Structural imaging

MRI scans yielded conclusive results as to the exclusion of other pathologies and the confirmation of diagnosis. One patient had a lenticulostriate infarct but was however classified as a sDAT patient. No significant correlation was found between the rCBF deficits and the regional atrophy rating scores derived from the MRI scans. Vascular dementia patients had more white matter lesions than sDAT patients (10.5 vs. 2.2 ml) did, whereas the periventricular hyperintensities did not differ between groups. The total amount of periventricular white matter hyperintensities correlated significantly with the memory performance on the AVLT and the MMSE score ($p = 0.02$ and 0.03 respectively; Spearman correlation coefficient).

⁵⁷Co SPECT scans

By visual analysis, ⁵⁷Co SPECT scans were unable to show any regional raised uptake (and in this way inflammatory lesions), irrespective of the disorder, depth or extent of the associated lesions on the perfusion images or MRI, and irrespective of the results of the NPT.

Perfusion SPECT - Neuropsychological testing

Perfusion SPECT scans in sDAT patients showed significant deficits in the anterior, superior and inferior mesiotemporal region, the inferior parietal region, the orbitofrontal, prefrontal, superior frontal and lateral frontal region, the posterior cingulate gyrus, the caput caudate nucleus, thalamus, and the cerebellum. A group perfusion defect for the sDAT patients was found in the left inferior parietal and the right temporal anterior region. The FLD patient showed perfusion deficits in the left lateral frontal and the right prefrontal region. The VaD patients showed mixed defects in the frontal, temporal and parietal lobes but also in the cerebellar region. The MMSE-score correlated significantly with the relative left temporal perfusion ($p = 0.002$, Pearson correlation coefficient). Results of the spatial orientation task correlated significantly with the relative perfusion in the right lateral frontal, right medial temporal and the right parietal region ($p = 0.03$, 0.005 , and 0.03 ; Pearson correlation coefficient).

DISCUSSION

Neuroinflammatory imaging

Scintigraphic visualisation of inflammation has previously been done with Ga⁶⁷, radiolabelled leukocytes, nanocolloid and human immunoglobulins [30]. The application of these techniques in sDAT for the visualisation of the inflammatory process would pose several difficulties. Indeed, despite repeated efforts by several laboratories, neutrophil invasion has until now not yet been documented in sDAT and a consistent lymphocytic or immunoglobulin involvement appears to lack [31]. The absence of these phenomena makes the application of the former mentioned techniques inadequate. As such, the aim of the present study was to visualise inflammatory lesions in sDAT patients with ⁵⁷Co SPECT and compare this with findings in patients suffering from other types of dementia. Inflammation as a pathogenic mechanism has been described to a lesser extent for VaD but not for FLD [32]. The evidence of inflammation in the group of frontotemporal dementia patients is to our knowledge limited to one study where some cases of Pick's disease were found to exhibit a neuronal expression of class II major histocompatibility complex with a dramatic microglial response suggesting an inflammatory process [33].

Limitations of the study

The limitations of ⁵⁷Co SPECT are manifold. Due to the long physical half-life of 270 days, only a limited dose can be injected which is responsible for the low count rate and the resulting low statistics. Moreover, whether ⁵⁷Co visualises specific aspects of neuronal damage or blood-brain barrier integrity is still uncertain. To what extent ⁵⁷Co really visualises calcium-mediated processes (*in vitro* and more importantly *in vivo*), and therefore resembles identical molecular uptake mechanisms, has yet to be determined, although the cerebral uptake of intravenously administered radioactive ⁴⁵Ca and ⁶⁰Co in neuronal damage is highly similar [7]. Finally, the exact cellular site of accumulation of radioactivity is, as yet, not known. As for inflammatory imaging, however, it is interesting to note that calcium may also accumulate in activated leukocytes and that both for ⁵⁵Co and ⁵⁷Co, only 12% of the total fraction is in its free form where the remainder is bound to leukocytes or plasma proteins [34-36].

Perfusion SPECT and sDAT

The role of perfusion SPECT in dementia, both for clinical (early diagnosis and follow-up) and research objectives has been well described in literature, even in the very early stages of the disease [37]. As such, the Therapeutics and Technology Assessment Subcommittee of the American Academy of Neurology evaluated the use of perfusion SPECT for sDAT as *established to support the clinical diagnosis* with a sensitivity of up to 95% [38]. Perfusion defects in sDAT patients have been mainly described in the posterior temporal and parietal lobe region, in concordance with the group perfusion defect in the temporal and parietal region found in this series. The frontal association cortex is said to be mostly unaffected until late in the course of the disease, however, this is contested by several SPECT and PET studies [38-40]. In this way, none of the dementia diseases can be identified with certainty by any characteristic topography of regional cerebral blood flow deficits, with an incidence of an exclusive or predominant bilateral reduction of perfusion tracer uptake in the

temporoparietal cortex ranging in literature from 26 to 100% [37, 41-43]. As such, group comparisons provide less information due to the heterogeneity of the disease (different stages and progression patterns), as already pointed out by Waldemar et al. [37].

Perfusion SPECT and other types of dementia, correlation with neuropsychological tests

The frontal perfusion defects found in the FLD patient is in agreement with the finding of Risberg et al. where bilateral frontal or frontotemporal defects were found in 25 out of 26 autopsy-verified cases of frontal lobe degeneration of the non-Alzheimer type [44]. Moreover, Pickut et al. identified bifrontal hypoperfusion as the most powerful predictor of clinical classification of sDAT versus FLD on perfusion SPECT [45]. The defects in the cerebellar region in the VaD patient are probably caused by functional diaschisis related to deafferentiation, where metabolic findings in any specific brain region represent complex relationships between a local and remote pathology. [46, 47]. The significant correlation between the orientation task and parietal perfusion confirms previous reports of this parietal hypoperfusion being associated with deficits in visuospatial function whereas a correlation between the MMSE-score and the relative temporal lobe perfusion was also described by O'Brien et al. [48] and Waldemar et al. [49].

MRI and sDAT

Not or only a partial correlation (right parietal region) was found between the rCBF deficits and the regional atrophy rating scores or the number of white matter lesions found on MRI. This is in agreement with studies performed by Eagger et al. and Waldemar et al. which indicates firstly that the hypoperfusion really reflects a reduced metabolism per gram brain tissue and secondly is not caused by a deafferentiation from underlying white matter hyperintensities [40, 50, 51]. The relationship between periventricular hyperintensities and cognitive functions as indicated in this study was already pointed out by Harrel et al [52]. Also, VaD patients having significantly more white matter lesions but not periventricular hyperintensities compared to sDAT patients, was previously indicated by Bowen et al. [53]. Although MRI is useful in the workout of patients with dementia since it shows the presence of space-occupying lesions, ventricular dilatation, cerebral atrophy, widening of sulci or infarcts, this technique is not of particular value in the direct diagnosis of sDAT, although promising results have been made with volumetric measurements of the (para)hippocampal and amygdala region [54].

Conclusions

In conclusion, ⁵⁷Co SPECT scans are not able to show any regional raised uptake and in this way ongoing tissue decay or inflammation, irrespective of the type of dementia, the depth or extent of perfusion defects, the presence of atrophy on MRI, or the results of NPT.

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CHAPTER FOUR

DEVELOPMENT AND VALIDATION OF RADIOLABELLED PK11195 FOR SINGLE PHOTON EMISSION COMPUTED TOMOGRAPHY

BIODISTRIBUTION AND DOSIMETRY OF [¹²³I]iodo-PK 11195: A POTENTIAL AGENT FOR SPET IMAGING OF THE PERIPHERAL BENZODIAZEPINE RECEPTOR

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ABSTRACT

The peripheral benzodiazepine receptor (PBR) is found in highest concentrations in kidneys and heart. In addition, it was reported to reflect neuro-inflammatory damage by a colocalisation with activated microglia. PK 11195 is a high affinity ligand for the PBR. The aim of the present study was to investigate in humans the biodistribution and dosimetry of [¹²³I]iodo-PK 11195, a potential SPET tracer for the PBR. Five healthy volunteers were injected with 112 MBq of ¹²³I labelled iodo-PK 11195. Sequential whole body scans were performed up to 72 hours post-injection. Multiple blood samples were taken, and urine was collected to measure the fraction voided by the renal system. Decay corrected ROIs of the whole-body images were analysed, and geometric mean count rates were used to determine organ activity. Organ absorbed doses and effective dose were calculated using the MIRD method. [¹²³I]iodo-PK 11195 was rapidly cleared from the blood, mainly by the hepatobiliary system. Approximately 22% was voided in urine after 48 hours. Average organ residence times were 0.74, 0.44, and 0.29 hrs for the liver, upper large intestine, and lower large intestine respectively. The testes received the highest dose, 109.4 μGy/MBq. All other organs investigated received doses of less than 50 μGy/MBq. The effective dose was 40.3 μSv/MBq. In conclusion, ¹²³I labelled iodo-PK 11195 can be used for the visualisation of the PBR and indirectly for the imaging of neuroinflammatory lesions. Taking into account the radiation burden of 7.46 mSv following an administration of 185 MBq, a ¹²³I labelled iodo-PK 11195 investigation has to be considered as an ICRP risk category IIb investigation.

INTRODUCTION

The central-type benzodiazepine receptor (CBR) with the known clinically relevant anxiolytic, anticonvulsant and muscle-relaxant effect of benzodiazepines is coupled to GABA receptors and their associated chloride channels. Unexpectedly, rat peripheral tissues used as negative controls for radioligand binding experiments also demonstrated high affinity [³H]diazepam binding [1]. These peripheral binding sites were structurally and pharmacologically distinct from the CBR. Based on their localisation outside of the central nervous system and the high affinity for several 1,4-benzodiazepines, these sites were designated "peripheral-type" benzodiazepine receptors (PBR) [2]. Although present in virtually all mammalian peripheral tissues, marked differences in PBR density and distribution of various species have been shown using autoradiographic techniques [3,4]. It is found in highest concentrations in kidneys, colon membranes, heart, steroid hormone producing cells of adrenal cortex, ovaries and testes, and several cell types of the immune system, such as mast cells and macrophages [2,5-7]. It is also present in low concentrations throughout the brain, primarily associated with the choroid plexus, ependymal linings, and glial cells [8-10]. Subcellular, the PBR is found in greatest abundance in the mitochondrial outer membrane and plasma membrane, however, other localisations are possible. Although the specific function of the PBR remains unknown, it is generally accepted to be involved in lipid metabolism and/or transport, heme biosynthesis, cell proliferation, or ion channel functions [2,11,12].

The immunomodulatory role for this receptor includes the ability to induce monocyte chemotaxis [13], modulate cytokine expression and superoxide generation [14], and stimulate formation of antibody-producing cells [6,15]. Moreover, it has the ability to reflect the effect of neuronal injury and neurotoxicity, by a colocalisation with activated microglia (brain resident macrophages) [16-18].

Iodo-PK 11195 [1-(2-iodophenyl)-N-methyl-N-(1-methyl-propyl)-3-isoquinolone carboxamide] is a specific and selective high affinity ligand (K_D 8.0 ± 1.7 nM) for the PBR in all species, comparable with PK 11195 itself (K_D 14.0 ± 3.4 nM) and, in this way, can be used as a diagnostic marker for the PBR. It has neither anxiolytic nor spasmolytic activity, nor interactions with other receptors and has thermodynamically been classified as an antagonist or partial agonist [2]. In vitro work revealed that iodinated PK 11195 binds specifically to the PBR, a binding that was dramatically increased at the sites of brain lesions [19].

In vivo visualisation of the human PBR, and in this way of glial neoplasms, neuronal damage, cellular inflammatory infiltration and microgliosis, has previously been done with ¹¹C radiolabelled PK 11195 [20-28]. Research with this ligand, however, is restricted to institutions with a positron emission tomography (PET) system and an in-house cyclotron that have access to these short-lived positron emitters. Therefore, the availability of a radiolabelled single photon emission computed tomography (SPET) ligand for the study of the PBR would allow a wider application. Similarly, Chalon et al. concluded already that iodinated PK 11195 could be suitable to detect brain injuries in humans by SPET [19].

In a previous study, the *in vivo* behaviour in mice (biodistribution, displacement and metabolism) and humans (metabolism) was assessed [29]. In the present study, the *in vivo* biodistribution and radiation dosimetry of [¹²³I]iodo-PK 11195 following a single intravenous-bolus administration was investigated in 5 healthy volunteers. The [¹²³I]iodo-PK 11195 blood and plasma pharmacological profile was determined. Data obtained from the biodistribution combined with basic pharmacokinetics of [¹²³I]iodo-PK 11195 were used to work out the dosimetry of [¹²³I]iodo-PK 11195 according to the MIRD formulation [30].

PATIENTS AND METHODS

Radionuclide synthesis and quality control

^{123}I was purchased from Amersham Cygne (the Netherlands) and PK 11195 was obtained from RBI (USA). ^{123}I labelled 1-(2-iodophenyl)-N-(1-methyl-propyl)-3-isoquinoline carboxamide (^{123}I jodo-PK 11195) was synthesised according to the method described previously [29,31], using a direct displacement of aromatic chlorine under solid-state conditions. The specific activity of the labelled compound was 6.7-17.6 GBq/ μmol (180-475 mCi/ μmol). The total labelling yield was 50-60% and the radiochemical purity of the final product, as assessed with high performance liquid chromatography (HPLC), was >99%.

Subject accrual and assessment

The study protocol was approved by the Institutional Review Board of the University Hospital. Five healthy volunteers (with regard to medical history and physical examination) consisting of 4 males and 1 female, with a mean weight of 72.4 kg (range 55 to 94 kg), and a mean age of 30.2 years (range 19 to 56 yrs) gave written informed consent. None of them had a clinical history that could have affected the biodistribution or elimination of the radioligand. Thyroid was blocked with Lugol's solution for all volunteers (5% iodine and 10% potassium iodide; one-day protocol of 20 drops one hr before the radioligand injection).

Administered activity measurements

The amount of radioactivity in each syringe containing ^{123}I jodo-PK 11195 was measured in a dose calibrator before and after injection. The mean dose administered was 112 MBq with a range of 51.8 to 181.7 MBq (1.7-4.9 mCi).

^{123}I jodo-PK 11195 gamma camera emission images

Scanning was done with a two-headed large-field-of-view gamma camera system (Helix, GE Medical Systems, Milwaukee, USA) equipped with a medium energy, general purpose, parallel-hole collimator (256 \times 1024 byte-mode matrix). A 20% photopeak window was symmetrically centred on 159 keV. The volunteers were lying supine with a 0.9% saline infusion (Baxter, Belgium) in the left arm (where blood sampling was performed), while the ^{123}I jodo-PK 11195 was injected in bolus via a peripheral right arm vein. Sequential anterior and posterior whole body scans were performed immediately post-injection and at 0.5, 1, 1.5, 2, 6, 24, 48 and 72 hours post-injection, with a scan speed varying from 12 cm/min for the early to 6 cm/min for the late images. The mean number of total counts of the first scan was 536 kcts in the AP- and 473 kcts in the PA-direction. Conversion from counts to activity was performed based on the initial whole body scan.

Pharmacokinetics and metabolite analysis

Blood samples (citrate tubes) were taken immediately post-injection and 15, 30, 45 sec, 1, 1.5, 2, 3, 5, 7.5, 10, 15, 20, 36, 50, 90 min, 4, 8, 24, 48 h post-injection. Radioactivity was determined with a 3 \times 3" NaI (TI) detector. The amount of radioactivity in the blood was calculated using total blood volume based on the individual haematocrit and expressed as % of injected activity of ^{123}I jodo-PK 11195. Urine was collected up to 48 hr to measure the fraction of the activity voided by the renal system. Activity not excreted in urine was assumed to be eliminated in faeces. Radioactivity in urine was measured using a well-type ionisation chamber (Radcal Corporation, Monrovia, USA). Analysis of metabolites in plasma and urine was performed with a HPLC system, as described previously [29].

Count rate measurements and organ residence times

Irregularly shaped regions of interests (ROIs) were drawn with a digital track ball along the outer border of those organs that accumulated sufficient activity to be seen clearly on the images. All ROIs were drawn by a single operator, minimising variability in region definition. The ROI set, determined in the anterior image with the best visualisation of the specific organ, was applied to all images, after translation to correct for any difference in subject position at the different acquisition times. Finally, ROIs were mirrored about their long axis for the posterior whole body images. Shapes and sizes were kept constant for all individual emission images. Decay corrected ROIs of the whole-body images were analysed and geometric mean count rates were used to determine source organ time-activity curves. A soft tissue region in the upper thigh was used for background subtraction. A multi-exponential fit was applied to the time-activity curves for the organs and tissues of each subject using in-house software. Residence times of the gall bladder, heart wall, liver and testes were calculated for each of the 5 volunteers. The residence time of the urinary bladder was calculated using the dynamic bladder model of Cloutier et al. with a voiding interval of 4.8 h [32]. For each volunteer the measured fraction of the activity leaving through the kidney – bladder pathway was taken into account. Residence times of the gastrointestinal tract were determined assuming the *ICRP 30* model. The gallbladder was assumed to empty its content every 6 h into the small intestine. Using the obtained individual residence times, target organ absorbed doses and effective dose were calculated using the MIRD method (3.0 software package) [30] with organ weighting factors from *ICRP 60* [33].

RESULTS

Pharmacokinetics and metabolite analysis

Figure 1 shows the percentage of the injected activity of [^{123}I]iodo-PK 11195 in whole blood, plasma, and plasma corrected for metabolites up to 60 minutes post-injection for one subject.

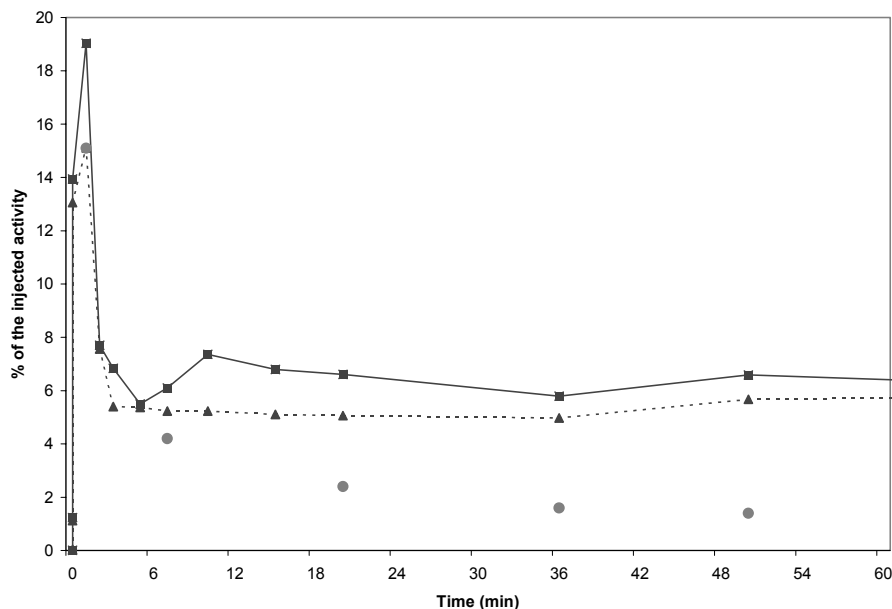


FIGURE 1. Percentage of the injected activity of [^{123}I]iodo-PK 11195 in whole blood, plasma, and plasma corrected for metabolites up to 60 minutes post-injection for one subject

■ whole blood; ▲ plasma; ● plasma corrected for metabolites

The [^{123}I]iodo-PK 11195 was rapidly cleared from the blood pool, primarily by the hepatobiliary system. An average of $77.5 \pm 10.2\%$ (range 60.0 to 85.3%) of the administered tracer remained in the soft tissues, which necessitated the background subtraction, especially for small organs.

Analysis of the metabolites in plasma showed a decomposition of the original tracer into two polar metabolites. Figure 2 shows the time course for the average percentage of parent radioactivity of [^{123}I]iodo-PK 11195 and the two major metabolites in venous plasma immediately post-injection, 7.5, 20, 37 and 50 minutes post-injection.

The mean measured urinary excretion was $22.0 \pm 3.2\%$ (range 18.9 to 25.2%) of the administered activity at 48 hr post-injection. No unchanged [^{123}I]iodo-PK 11195 was detected in urine.

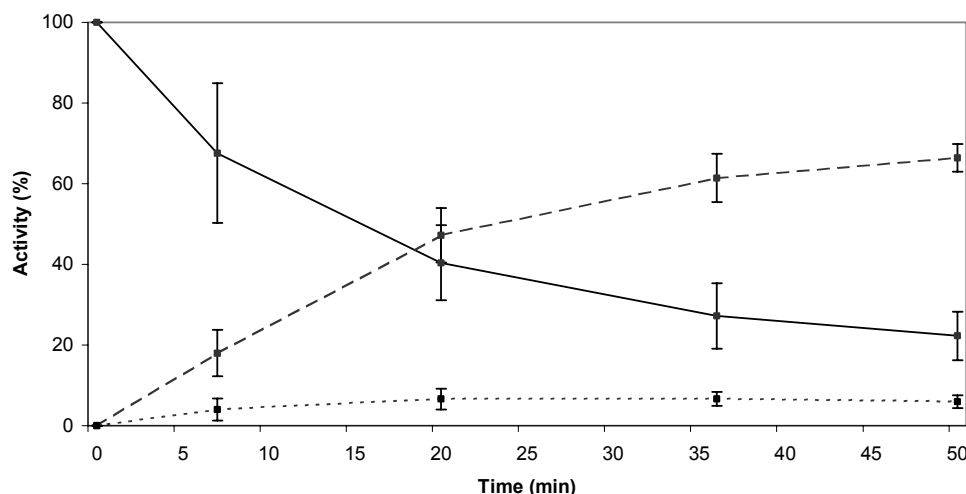


FIGURE 2. Time course for the average percentage (\pm SD) of parent radioactivity of [^{123}I]iodo-PK 11195 and two major metabolites in venous plasma immediately post-injection, 7.5, 20, 36 and 50 minutes post-injection from five individuals studied.

_____ [^{123}I]iodo-PK 11195
 - - - - - major metabolite (probably free ^{123}I)
 other metabolite

Biodistribution and dosimetry

All subjects completed successfully the imaging protocol. No adverse or subjective effects of the tracer on any of the subjects were observed. Serial anterior whole body images of one subject are presented in Figure 3. Visual analysis of the acquired body scans showed avid and rapid liver uptake of the radiopharmaceutical. Activity noted within the gall bladder and bowel provides clear evidence of excretion through the enterohepatic route. No other major organ systems showed significant uptake of [^{123}I]iodo-PK 11195, except for some activity in the heart (average uptake 1.9%, highest uptake 3.1% immediately post-injection) and a small amount of activity in the testes for 2 of the 4 males (average uptake 0.5%, highest uptake 0.6% 7 hr post-injection) and thyroid for 3 subjects (average uptake 0.4%, highest uptake 0.7% 24 hr post-injection). Figure 4 displays the time-activity curves for heart, liver, gallbladder and testis for one subject. Concerning the equilibrium concentrations of tracer (%/ID/g) in various tissues, the following levels for the specific uptake were obtained in the steady-state situation two hours after administration: liver 4.5×10^{-3} %/ID/g ($\text{SD}=0.5 \times 10^{-3}$), heart 9.7×10^{-3} %/ID/g (1.3×10^{-3}) and testes 2.7×10^{-2} %/ID/g (0.5×10^{-2}).

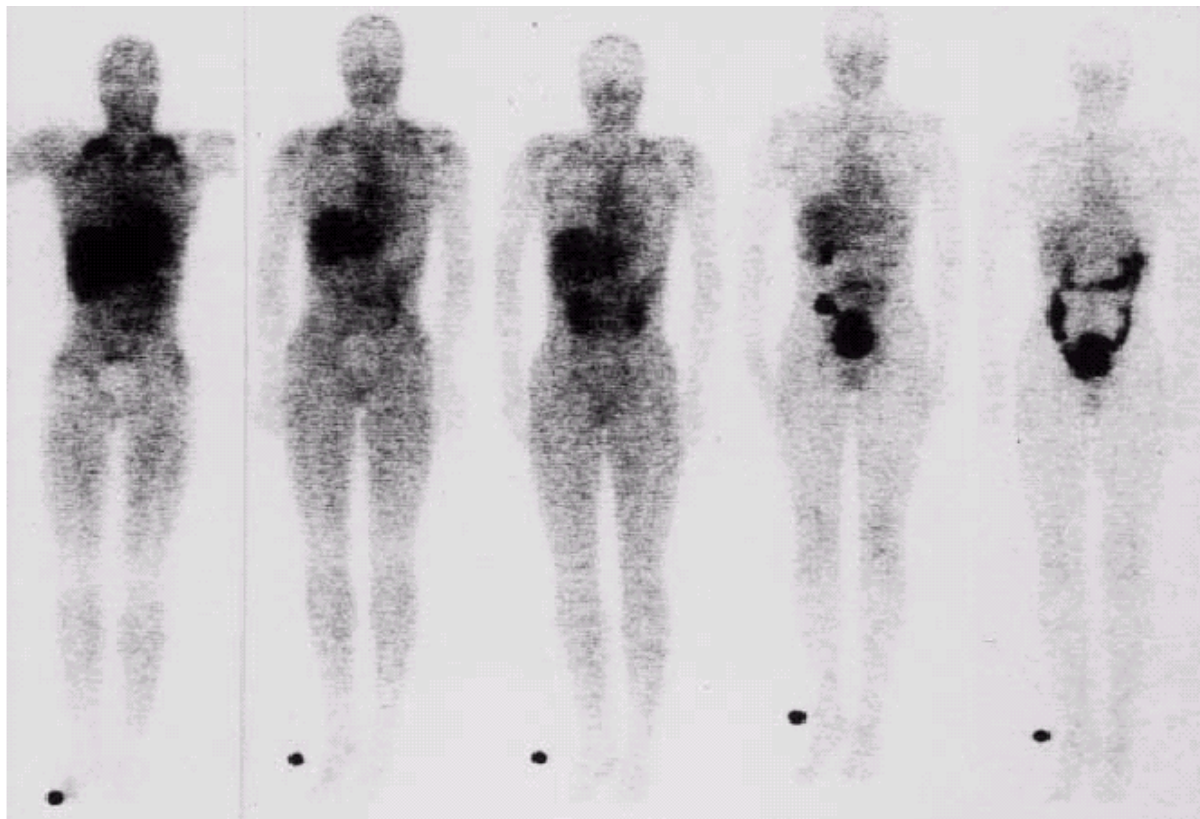


FIGURE 3. Serial anterior whole body images immediately post-injection, 1, 2, 6 and 24-hr post-injection. An intense gallbladder activity is seen on the 6-hr images along with activity in the liver and large bowel system. On the 2-hr images both kidneys can be clearly visualised

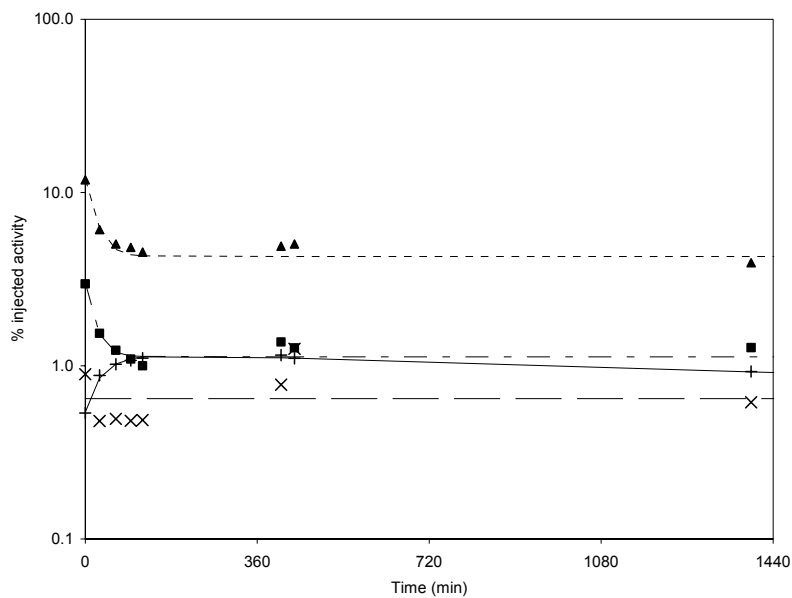


FIGURE 4. Time-activity curves for liver, heart, gallbladder and testis for one subject (expressed as % of the injected activity) ▲ Liver (----- fit line); ■ Heart (--- fit line); × Gall bladder (— fit line); + Testes (—— fit line)

Table 1 shows the residence times for each of the 5 volunteers. Except for the remainder compartment, the values were highest for the liver in all subjects. Average organ residence times were 0.74 ± 0.18 hr (range 0.47 to 0.87 hr), 0.44 ± 0.29 hr (range 0.15 to 0.76 hr), and 0.29 ± 0.19 hr (range 0.10 to 0.49 hr) for the liver, upper large intestine, and lower large intestine respectively. Average organ residence time of the testes (4 male volunteers) was 0.17 ± 0.03 (range 0.12 to 0.19 hr). For the one female volunteer the ovary residence time was estimated, based on literature data, assuming a similar specific activity (activity/g) as in the testes [5,34-36]. This procedure was necessary because of the impossibility to draw ROIs in the ovary region due to the superimposed gastrointestinal tract. For testes and ovaries mass, standard values were adopted [37].

TABLE 1. Residence times (hr) in each organ for all subjects

Organ	Subject				
	1	2	3	4	5
GB	0.17	0.15		0.12	0.25
SI	0.12	0.09	0.35	0.34	0.47
ULI	0.20	0.15	0.56	0.54	0.76
LLI	0.13	0.10	0.36	0.35	0.49
Heart wall	0.24	0.39	0.36	0.22	0.17
Liver (* +GB)	0.47	0.85	*0.80	0.71	0.87
UB	0.23	0.22	0.20	0.23	0.27
Testes/Ovaries *	0.12	0.19	0.19	0.18	*0.05
Remainder	15.50	15.30	16.20	15.20	14.10

GB = gallbladder; LLI = lower large intestine; SI = small intestine; ULI = upper large intestine; UB = urinary bladder

Table 2 lists the absorbed dose estimates and effective dose for [^{123}I]iodo-PK 11195 in this sample. The testes received the largest radiation burden: $109.4 \pm 19.3 \mu\text{Gy}/\text{MBq}$. Gallbladder wall, upper large intestine and lower large intestine received doses of respectively 48.7 ± 19.4 , 39.9 ± 16.2 and $38.3 \pm 14.8 \mu\text{Gy}/\text{MBq}$. The ovary dose was estimated to be $138.0 \pm 24.3 \mu\text{Gy}/\text{MBq}$. All other organs investigated received doses of $31.5 \mu\text{Gy}/\text{MBq}$ or less. The mean effective dose for the normal adult was estimated to be $40.3 \pm 6.6 \mu\text{Sv}/\text{MBq}$.

TABLE 2. Radiation absorbed dose estimates for [^{123}I]iodo-PK 11195

Target organ	Mean ($\mu\text{Gy}/\text{MBq}$)	Standard deviation
Adrenals	16.2	0.6
Bone surfaces	23.7	1.0
Brain	11.7	0.6
Breasts	10.1	0.5
Gallbladder wall	48.7	19.4
Heart Wall	31.5	7.8
Kidneys	15.2	0.6
Liver	21.9	3.4
LLI wall	38.3	14.8
Lungs	14.2	0.7
Muscle	13.1	0.6
Ovaries	138.0	24.3
Pancreas	17.5	0.5
Red marrow	13.0	0.6
Skin	9.1	0.4
Small intestine	24.9	6.8
Spleen	14.7	0.6
Stomach	15.8	0.7
Testes	109.4	19.3
Thymus	14.0	0.9
Thyroid	13.4	0.7
Total body	14.3	0.7
ULI wall	39.9	16.2
Urinary bladder wall	29.9	1.6
Uterus	19.4	1.5
Effective dose ($\mu\text{Sv}/\text{MBq}$)	40.3	6.6

LLI = lower large intestine; ULI = upper large intestine

DISCUSSION

The present study is the first study to describe the biodistribution and dosimetry of radiolabelled PK 11195 for SPET in humans. Although several reports described the use of [^{11}C]PK 11195 in various diseases, there has been to date no report of a biodistribution, dosimetry or quantitative compartmental modelling of [^{11}C]PK 11195 data because of inconsistent plasma data hampering the application of quantification methods that rely on establishing a plasma input function, the lack of procedures for the determination and quantification of circulating radiolabelled metabolites in healthy volunteers and the lack of a “reference” brain region devoid of specific signal. Recently however, a cluster analytical approach, that functionally extracts a distinct kinetic component representing normal ligand kinetics, was proposed as a viable means of generating an input function to the simplified reference tissue model in the analysis of [^{11}C]PK 11195 clinical data [38]. Thus, in normal brain tissue, only the use of a saturation procedure (coinjection with saturating amounts of cold PK 11195) has been able to demonstrate the specific binding of [^{11}C]PK 11195, but its precise quantification was complicated due to the displacement, and subsequent release into the systemic circulation, of radiotracer bound specifically to peripheral organ tissues, resulting in transiently enhanced uptake in the brain [39]. In this way, Petit-Taboué et al. and Sette et al. performed challenge studies in baboons with saturating doses of cold ligands which confirmed the specific *in vivo* binding, both in the unlesioned, physiological state as after focal induced ischaemia [40,41].

[^{123}I]iodo-PK 11195 appears to be a radiopharmaceutically safe radioligand and did not produce any subjective or objective pharmacological effects in human volunteers in this series. This is consistent with literature since PK 11195 was not reported to have a perceptible effect on humans, certainly in the nanomolar dose range administered as a radioligand [2,42].

The biodistribution of radiolabelled iodo-PK 11195 has previously been described in mice [29,43], rats, and dogs [44]. In rats, the tracer exhibited preferential accumulation in organs known to be high in PBR density, such as heart and especially adrenal gland. This accumulation could be decreased with as much as 87% by pre-treatment of rats with 5 mg/kg cold PK 11195 [31]. Similarly, Hashimoto et al. found that the radioactivity after administration of ^3H -PK 11195 in mice was significantly decreased by the coadministration of carrier PK 11195 [43]. In none of the subjects in the present study, however, an uptake of activity was seen in the adrenal gland. In dogs, the highest activity was found in bile [44], which is consistent with the observed activity in gallbladder in the present study. Moreover, the secondary peak in plasma concentration noted in one volunteer at approximately 24 hrs can be explained by an enterohepatic recycling phenomenon, as previously described by Ferry et al. [42].

From the first hr up to 24 hr post-injection, testis activity could be clearly seen in 2 of the 4 males, which is consistent with the known presence of PBRs in the Leydig secreting cells of the testis. This testis activity is reflected in the rather high gonadal dose with this dose contributing primarily for 57% to the effective dose. However, the estimated dose received by the ovaries is probably an overestimation due to the fact that, although not properly compared in humans and given the influence

of various endocrine and paracrine hormones, the number of peripheral benzodiazepine receptors in human ovaries is probably not as high as in testes, corresponding to the fact that the ovaries could not be traced on the whole-body sections [34,45,46]. In this way, the assumption of a similar specific activity in ovaries as in testes has probably made us overestimate the dose. Moreover, one has to take into consideration that [^{123}I]iodo-PK 11195 will be predominantly used in patients with neurodegenerative diseases outside the reproductive age range.

Also, thyroid showed significant accumulation of the tracer in 3 of the 5 subjects on the late images, despite thyroid blockage with Lugol's solution. In spite of the presence of PBRs in thyroid tissue [44], the uptake of radioactivity at this time point most likely reflects the uptake of free iodide resulting from the *in vivo* dehalogenation.

Previous metabolite analysis in mice showed a dramatic metabolisation of [^{123}I]iodo-PK 11195 in blood ($\pm 55\%$) within 2.5 minutes, with the major metabolite most likely being free ^{123}I . In brain and heart however, the only radioactive compound found was the original product [29], probably due to the fact that the major metabolites do not enter the heart and brain. Similarly, Hashimoto et al. found no radioactive metabolites in heart, lung and brain 20 minutes after intravenous administration of ^3H -PK 11195 [43]. In spite of this rapid metabolisation, the absence of radioactive metabolites in the organs mentioned above makes this an appropriate radioligand to study peripheral benzodiazepine receptors in man. Also, the specific activity of [^{123}I]iodo-PK 11195 is comparable with the specific activity of [^{11}C]PK 11195 (18.5-74 GBq/ μmol) required for quantitative PET studies as stated by Pike et al. [47].

A rapid penetration of an intact blood-brain barrier is possible, as the level of radioactivity in brain of mice exceeded the one in blood 40 sec. after injection, and thereafter, rapidly cleared from cerebral tissue, with radioactivity levels decreasing below blood levels 10 min. after injection [29]. This rapid rise in cortical and grey matter activity has also been demonstrated by Petit-Taboué et al. with [^{11}C]PK 11195 in baboons [40]. Likewise, Banati et al. showed an increased PK 11195 binding to activated microglia after facial nerve axotomy - a lesion causing a retrograde neuronal reaction without nerve cell death while keeping the blood-brain barrier intact - where the peak of PK 11195 binding was observed 4 days after the peripheral nerve lesion, which is consistent with the well-known time course of microglial activation. Moreover, photoemulsion microautoradiography confirmed the restriction of PK 11195 binding to activated microglia, where the full transformation of microglia into parenchymal phagocytes is not necessary to reach maximal levels of PK 11195 binding. The authors concluded that PK 11195 is a well-suited marker to detect microglial activation in areas of subtle brain pathology, where neither a disturbance of blood-brain barrier function nor the presence of macrophages and inflammatory cells indicate an on-going disease process [48]. In the present study, the highest brain uptake was approximately $2.0 \pm 0.5\%$ (range 1.0 to 3.1%), which is expected due to the low concentration of PBRs throughout the brain in healthy volunteers.

Probably, the agent is not appropriate for SPET imaging of the gastrointestinal tract due to the main excretion by the gastrointestinal system and the high abdominal activity. Even so, [¹²³I]iodo-PK 11195 seems theoretically promising for imaging of the heart, due to the electrophysiological and pharmacological evidence that PBRs are coupled to calcium channels in the heart [49]. However, cardiac imaging may prove difficult, due to the large liver and gallbladder uptake.

These findings suggest that [¹²³I]iodo-PK 11195 can be used safely in clinical investigations of the PBR for the imaging of neuroinflammatory lesions. The radiation absorbed doses are low enough to allow 185 MBq of activity to be administered to a healthy volunteer during each study, giving an average effective dose of 7.46 mSv. This administered dose is comparable with other [¹²³I]labelled receptor ligands as β -CIT, FP-CIT and IBZM [50,51]. For quantitative PET studies with [¹¹C]PK 11195, 185-888 MBq is required to be injected intravenously [26,27,47].

Concerning the proper imaging time post-injection, no dynamic SPET scans were performed in the present study, but a period of 30 to 90 minutes post-injection seems adequate. Indeed, Sette et al. noticed stable [¹¹C]PK 11195 uptake ratios across various gray matter structures analysed as early as 20 minutes after injection with no significant relation between [¹¹C]PK 11195 uptake and corresponding cerebral blood flow ratios between 20 and 60 minutes post-injection [41]. Likewise, Pappata et al found in a patient with a glioblastoma a tumor/normal gray matter ratio of 2.12 at 10 min which remained quite constant until the end of the study (60 min post-injection) [21].

CONCLUSIONS

¹²³I labelled iodo-PK 11195 is a suitable agent for the visualisation of the PBR and indirectly for the imaging of neuroinflammatory lesions. Taking into account the acceptable radiation burden of 7.46 mSv following an administration of 185 MBq, a ¹²³I labelled iodo-PK 11195 investigation has to be considered as an ICRP risk category IIb investigation with minor to intermediate risk, requiring a moderate benefit [52].

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CHAPTER FIVE

VALIDATION OF RADIOLABELLED PK11195 AS AN INFLAMMATORY TRACER IN
MULTIPLE SCLEROSIS

MULTIPLE SCLEROSIS

Multiple Sclerosis (MS) is the prototype inflammatory autoimmune disorder of the central nervous system and, with a lifetime risk of one in 400, potentially the most common cause of neurological disability in young adults. As with all complex traits, the disorder results from an interplay between as yet unidentified environmental factors and susceptibility genes. Together, these factors trigger a cascade of events, involving engagement of the immune system, acute inflammatory injury of axons and glia, recovery of function and structural repair, post-inflammatory gliosis, and neurodegeneration. The sequential involvement of these processes underlies the clinical course characterised by episodes with recovery, episodes leaving persistent deficits, and secondary progression. The aim of treatment is to reduce the frequency, and limit the lasting effects, of relapses, relieve symptoms, prevent disability arising from disease progression, and promote tissue repair. Despite limited success in each of these categories, everyone touched by multiple sclerosis looks for a better dividend from applying an improved understanding of the pathogenesis to clinical management.

The present part reviews the history, epidemiology, pathophysiology, clinical features and disease course, and treatment of MS.

HISTORY AND EPIDEMIOLOGY

Previously unrecognised, multiple sclerosis makes a fleeting appearance in the early 19th century before taking centre stage as clinical neurology began to flourish in the 1860s. By the beginning of the 20th century, a disease only a few years earlier meriting individual case reports had become one of the most common reasons for admission to a neurological ward. The incidence of MS is greatest at the extremes of latitude in both the northern and southern hemispheres (hence rarely observed in Asians or Africans) and affects almost twice as many women as it does men (at least in the most common relapsing remitting type of MS); this unexplained bias mimics that seen in other putative autoimmune diseases. The disease has an incidence of about seven per 100 000 every year, prevalence of around 50 to 150 per 100 000 for Caucasians, and a lifetime risk ranging from one in 1000 to one in 250. Now, multiple sclerosis is recognised throughout the world, with around 2.5 million affected individuals. These crude statistics conceal the harsh reality of a frightening and potentially disabling disease for young adults.

PATHOPHYSIOLOGY

The oligodendrocyte, a principal target of immune attack in multiple sclerosis, synthesises and maintains the myelin sheath of up to 40 neighbouring nerve axons in the central nervous system. Compact myelin consists of a condensed membrane, spiralled around axons to form the insulating segmented sheath needed for saltatory axonal conduction: voltage-gated sodium channels cluster at the unmyelinated nodes of Ranvier, between myelin segments, from where the action potential is

propagated and spreads passively down the myelinated nerve segment to trigger another action potential at the next node.

The consequences of demyelination for saltatory conduction explain many clinical and laboratory features of multiple sclerosis. Partially demyelinated axons conduct impulses at reduced velocity - explaining the characteristic delays in conduction of evoked potentials. Demyelinated axons can discharge spontaneously and show increased mechanical sensitivity - accounting for the flashes of light on eye movement (phosphenes) and electrical sensation running down the spine or limbs on neck flexion (Lhermitte's sign). Partially demyelinated axons, whose safety factor for conduction is compromised, cannot sustain the fall in membrane capacitance induced by a rise in temperature, and conduction fails - leading to the characteristic appearance of symptoms and signs after exercise or a hot bath (Uhthoff's phenomenon). Ephaptic transmission (cross-talk) can arise between neighbouring demyelinated axons, resulting in paroxysmal symptoms - trigeminal neuralgia, ataxia, and dysarthria, or painful tetanic posturing of the limbs, lasting one or two minutes and often triggered by touch or movement. Individuals with multiple sclerosis characteristically tire during physical and cognitive tasks, and take longer to recover: although poorly understood, and probably multifactorial, fatigue in multiple sclerosis can be very disabling, even in isolation.

The symptoms and signs of multiple sclerosis merely reflect the functional anatomy of impaired saltatory conduction at affected sites. The cerebrum is almost always involved when assessed with magnetic resonance imaging (MRI), but most white matter abnormalities cannot be linked to specific events or clinical symptoms, anyway, new lesions appear to occur at least seven to ten times more frequently than clinical attacks, where especially the correlation between T2 lesions and disability is poor (clinico-radiological paradox) [1]. Involvement of the anterior visual pathway is the rule. Lesions of the brainstem and cerebellar pathways produce precise clinicopathological correlations; typically, coordinated movement of the eyes, limbs, bulbar musculature, and axial muscles is disrupted. The spinal cord is frequently affected, leading to alterations in motor, sensory, and autonomic functions.

One hypothesis to explain the breakdown of immune regulation in autoimmune diseases is molecular mimicry, which suggests that a peptide (the environmental factor), presented in the groove of specific class II molecules (one component of inherited risk), is immunologically indistinguishable from self-antigen and, hence, an appropriate response to infection generates inappropriate inflammation against some component of the oligodendrocyte-myelin unit. Also, damage to normal tissue may expose novel antigens to the immune system that would otherwise not be contacted and further direct attack against nearby self-antigens, i.e. epitope spreading. In common with all organ-specific autoimmune diseases, this systemic defect results not in a sustained autoimmune attack on the entire target organ but, rather, in inflammatory lesions that are temporally and spatially segregated.

MOLECULAR GENETICS AND ENVIRONMENTAL FACTORS

Multiple sclerosis is caused by an interplay between genes and environment. There is a familial recurrence rate of about 15%. The age-adjusted risk is higher for siblings (3-5%), parents (2%), and children (2%) than for second-degree and third-degree relatives. Recurrence in monozygotic twins is around 25-35%. Recurrence is higher in the children of conjugal pairs with multiple sclerosis (20%) than in the offspring of single affecteds (2%). Conversely, the risk is not increased either for individuals adopted into a family with an affected individual or in the non-biological relatives of adoptees who themselves develop multiple sclerosis.

Multiple sclerosis seems to be genuinely polygenic in which the genes responsible for the complex traits are not mutations coding for aberrant gene products but normal polymorphisms [2]. They act independently or through epistasis, and each polymorphism can exert a small contributory effect on some as yet undefined structure or physiological function. Extensive searches have yielded few secure candidate regions. Results of population studies suggest an association between the human leucocyte antigen (HLA) class II MHC alleles which code for molecules that participate in antigen recognition by T lymphocytes and the gene for TNF- α encoded within the same linkage group. The list of candidate genes that have been screened includes many adhesion molecules, immune receptors or accessory molecules, cytokines and their receptors or antagonists, chemokines, growth promoting molecules, and structural genes of the myelin-oligodendrocyte unit. Disappointingly, the low yield from this trawl is not definitively advanced by eight whole genome linkage screens done in several countries [3]. In common with most other complex traits, no major susceptibility gene has yet been identified, although several promising chromosomal linkages are provisionally linked and associated with multiple sclerosis - at 1p, 6p, 10p, 17q, and 19q [4].

The distribution of multiple sclerosis cannot be explained on the basis of population genetics alone. Outside Europe, prevalence rates among white people are half those documented for many parts of northern Europe. In Australia and New Zealand, there are gradients in frequency that do not follow genetic clines. The risk is higher for English-speaking white people who migrate into South Africa as adults than as children. The low frequency of multiple sclerosis in Africans increases substantially for first-generation descendants raised in the UK. Results of surveys of multiple sclerosis have prompted speculation on the occurrence of epidemics in Iceland, the Orkney and Shetland Islands, and the Faroes (where MS was unknown until 1940 when British soldiers landed on its shores), although others prefer the interpretation that these merely indicate improved case recognition. There is age-linked susceptibility to viral exposure in those who are constitutionally at risk of developing the disease. Attempts to reliably implicate specific environmental agents are frustrating. Recent, yet unsubstantiated candidates, include *Chlamydia pneumoniae* [5], Epstein-Barr Virus, and human herpesvirus type 6 [6].

CLINICAL DIAGNOSIS

Revised diagnostic criteria classify individuals in the categories of multiple sclerosis, not multiple sclerosis, or possible multiple sclerosis, and incorporate evidence from MRI. As with the previous diagnostic criteria, individuals must have a minimum of two attacks, affecting more than one anatomical site, but, assuming an initial presentation suggestive of multiple sclerosis, the second lesion need not necessarily be clinically expressed [7].

Investigations are done for four main reasons in patients with multiple sclerosis: they allow to see the anatomical dissemination of lesions in time and space (imaging); they permit the assessment of intrathecal inflammation (spinal fluid analysis); they show that conduction has altered in a pattern consistent with demyelination (evoked potentials); and they allow the exclusion of conditions that mimic the disease.

More than 95% of patients with multiple sclerosis have T2-weighted white matter abnormalities, but these are not diagnostic. They occur about 10 times more frequently than new clinical events. Imaging is not necessary for diagnostic purposes in patients with a history of relapsing disease, affecting multiple sites within the central nervous system. The major practical use is in the investigation of individuals with clinically isolated lesions or progressive disease at a single site. There is less cerebral involvement in patients with primary progressive multiple sclerosis than in those who have comparable disability from secondary progression. Variations in imaging protocols are beginning to distinguish separate components of the underlying pathological process - inflammation (gadolinium DTPA enhancement of T1-weighted lesions, reflecting a breach in the normal blood-brain barrier and indicating that the lesion is of recent origin), demyelination (magnetisation transfer ratio), astrocytosis (T2-weighted lesions, the signal arising from increased water content), and axonal damage (reduction in diffusion tensor imaging anisotropy and N-acetyl-aspartate spectra with chemical shift imaging, or the presence of focal atrophy and T1-weighted black holes) [8].

Cerebrospinal fluid protein electrophoresis shows oligoclonal IgG bands in more than 90% of cases. Their role in the pathogenesis of multiple sclerosis is unresolved. Screening spinal fluid against cDNA expression, phage display, or random peptide libraries has not distinguished common antigen specificities; some antibodies are directed against components of the oligodendrocyte or its myelin membranes, and others recognise extrinsic antigens including viruses, but collectively these specificities only account for a minority of the bands. Diagnostically, spinal fluid oligoclonal bands confirm that the underlying pathology is inflammatory, which can be useful in excluding alternative explanations, especially in the context of progressive spinal cord syndromes and in elderly patients in whom imaging abnormalities are not discriminatory.

Demyelination characteristically delays the latencies of visual, auditory, and somatosensory evoked potentials, as well as central motor conduction times, leaving the amplitude of responses unchanged. Before the advent of MRI, these abnormalities provided evidence for clinically silent lesions; now, their

role is confined to the provision of circumstantial evidence for demyelination in diagnostically difficult situations, such as syndromes that progress from onset.

NATURAL HISTORY AND EVOLUTION OF THE PLAQUES

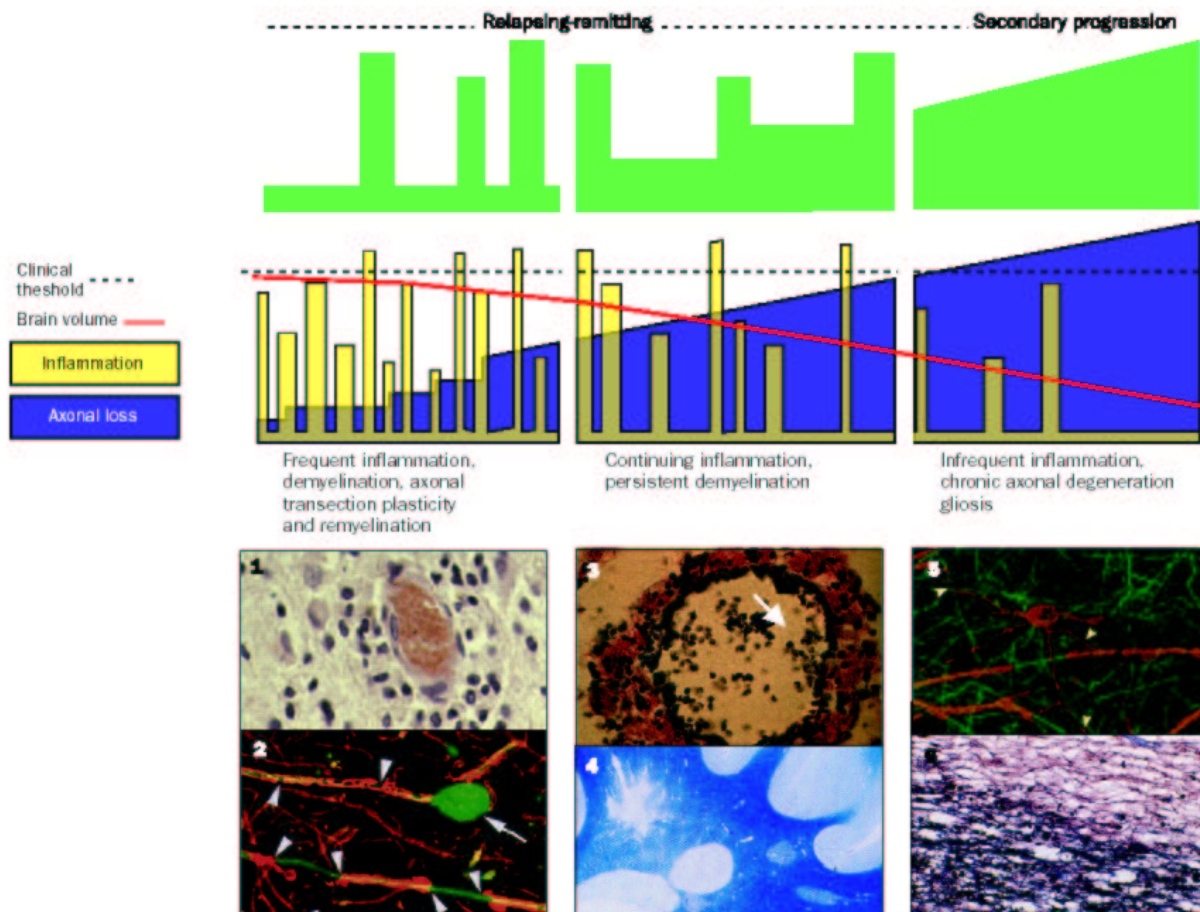
80-90% of patients present with relapsing - remitting disease and, typically, the illness passes through phases of relapse with full recovery, relapse with persistent deficit, and secondary progression. In about a quarter of patients, multiple sclerosis never affects activities of daily living; conversely, up to 15% become severely disabled within a short time. Episodes happen at random intervals, but initially average about one per year, decreasing steadily thereafter. In 10-20% of patients, the disease is progressive from onset, hence termed primary progressive - affecting the spinal cord and, less frequently, the optic nerve, cerebrum, or cerebellum. Disease onset is usually in the third or fourth decade, but 2% of patients with multiple sclerosis present before the age of 10 years, and 5% before age 16 years. In children, the distinction from acute disseminated encephalomyelitis can often only be established by observing the subsequent natural history. Overall, life expectancy is at least 25 years from disease onset with most patients dying from unrelated causes.

The prognosis is relatively good when sensory or visual symptoms dominate the course of multiple sclerosis in adults, and there is complete recovery from individual episodes. This pattern is most common in young women. Conversely, motor involvement, especially when coordination or balance are disturbed, has a less positive prognosis. The outlook is also poor in older men who develop the disease. Frequent and prolonged relapses with incomplete recovery at onset and a short interval between the initial episode and first relapse are adverse prognostic features [9], but the main determinant of disability is onset of the progressive phase [10].

Fixed disability in multiple sclerosis is acquired through two distinct mechanisms: incomplete recovery from relapse and disease progression. Patients with relapsing-remitting multiple sclerosis accumulate disability from disease onset more slowly than those with primary progressive multiple sclerosis. However, beyond a degree of disability sufficient to limit walking to less than 500 m without aid or rest (Kurtzke expanded disability status scale [EDSS] of 4.0), subsequent accumulation no longer correlates with mode of presentation, suggesting that the pathological substrate for progression determines disability at this stage of the disease [11].

Prospective studies show that around 10% of upper respiratory (adenovirus) and gastrointestinal infections, arising in patients with multiple sclerosis, are followed by relapse, and about 30% of new episodes relate to infection. There is no evidence that trauma causes multiple sclerosis, triggers latent disease in someone who has the underlying disease process, or alters the course in individuals who have already experienced symptoms. People with multiple sclerosis cope less well with symptoms while exposed to stress, but psychological factors do not directly affect disease activity.

Maturation of the individual lesion involves several stages: a) immune engagement, b) acute inflammatory injury of axons and glia, c) recovery of function and structural repair and d) post-inflammatory gliosis and neurodegeneration. Healthy individuals harbour autoreactive myelin T cells, normally kept in check by regulatory T cells. Failure of regulation leads to proliferation, activation, and entry into the circulation of autoreactive T cells; they express adhesion molecules and induce reciprocal changes in endothelia, allowing access across the blood-brain barrier into the central nervous system. There, activated T cells re-encounter antigen and activate microglia (the CNS macrophage); they, in turn, express HLA class II molecules, re-present antigen to T cells, and set up a proinflammatory loop, which provides an infiltrate rich in activated T cells and microglia with some neutrophils. On the figure below perivascular inflammation is shown (panel 1) which causes acute axonal transection (panel 2), and microglia-mediated removal of myelin (panel 3) with persistent demyelination despite some remyelination (panel 4); chronic lesions show further axonal loss (panel 5) and gliosis (panel 6). This scheme does not depict primary progressive multiple sclerosis in which there is pronounced axonal degeneration with or without a preceding inflammatory phase [12].



Toxic inflammatory mediators are released, sustaining breakdown of the blood-brain barrier and leading to injury of axons and glia. Nitric oxide might act directly on normal or hypomyelinated axons, transiently blocking conduction [13] and reversibly increasing deficits arising from already compromised pathways. Symptoms also improve as surviving functional pathways are reorganised at

the cellular [14] and systems level [15]. Together, these mechanisms account for remission early in the disease. But tissue vulnerability is easily exposed. When compounded by high axonal firing frequency, nitric oxide causes structural (and hence irreversible) changes to axons [16]. Axonal transection in acute inflammatory plaques is shown histologically [17] and radiologically through reduction in the neuronal spectroscopic marker, N-acetyl aspartate (NAA) [18]. These transected axons undergo Wallerian degeneration during the subsequent 18 months [19], but this action does not seem to extend the lesion or shape the clinical deficit.

Cytokines and growth-promoting factors released by reactive astrocytes and microglia as part of the acute inflammatory process promote endogenous remyelination. But, over time, astrocyte reactivity seals the lesion and gliosis causes a physical barrier to further remyelination, reducing the capacity to accommodate cumulative deficits, and marking transition to the stage of persistent deficit.

Most axonal loss is seen in secondary progressive multiple sclerosis [20]. It is proposed that chronic axonopathy is not due directly to inflammation nor does it occur only colocalised with discrete pathological lesions, but results from loss of trophic support normally provided to axons by myelin or glia, acting directly or through the maintenance of electrical activity, or both [21,22]. As such, chronic axonal degeneration might slowly increase the clinical deficit, decaying a compromised but functioning pathway and leading to disease progression.

TREATMENT

The aims of treatment are to: a) reduce relapse rates, b) prevent fixed disability directly attributable to relapse, c) provide symptomatic management of fixed neurological deficit, d) prevent disability acquired through progression, e) treat established progression.

Reducing relapse rates in multiple sclerosis

Since permanent disability can be caused by incomplete recovery from episodes, relapse frequency is bound to correlate with accumulation of disability during the relapsing-remitting phase of multiple sclerosis. The dividend from reducing the relapse rate is best shown by use of the β -interferons: interferon β -1a, and interferon β -1b. These type-1 interferons were first used in multiple sclerosis for their antiviral action, in view of the known propensity of viral infections to trigger relapses. Their predominant mechanism of action is unknown, but they have been found to suppress T cell proliferation, reduce T cell migration from the systemic circulation into the CNS, alter the T cell cytokine secretion repertoire from relatively proinflammatory Th1 to relatively anti-inflammatory Th2 response, and downregulate class II MHC antigen expression [23]. The annual relapse rate for individuals treated with interferon- β is significantly reduced by 30-37%, however, only with interferon β -1a this change in relapse rate is also accompanied by a reduction in the accumulation of disability [24].

Three other agents reduce relapse frequency, and the accumulation of disability, in relapsing-remitting multiple sclerosis; each has similar efficacy to the β -interferons and acceptable adverse effects profiles. Glatiramer acetate was noted serendipitously to suppress experimental allergic encephalomyelitis, the animal model of demyelinating disease, perhaps by inhibiting the binding of myelin basic protein (MBP) to the T cell receptor or by altering the phenotype of myelin-autoreactive T cells [25], and is able to reduce the annual relapse rate by 25% [26]. Secondly, azathioprine inhibits lymphocyte proliferation by inhibiting purine synthesis, and probably has similar efficacy to the β -interferons, although trial data were less clear-cut [27]. Thirdly, mitoxantrone inhibits DNA repair and synthesis in dividing and non-dividing cells through inhibition of DNA topoisomerase II; it is potentially much more toxic than the β -interferons, and is mainly used for the treatment of aggressive relapsing disease, including patients with high relapse frequency in the progressive phase [28].

Prevention of disability attributable to relapse

Mild attacks causing little or no functional impairment may require no treatment other than rest and often resolve spontaneously. Relapses causing functional impairment (e.g., visual loss, weakness, significant gait impairment) are typically treated with corticosteroids where they reduce the duration of relapses and hence their short-term morbidity, but not the ensuing permanent deficits. Corticosteroids, bound to their cytoplasmic receptors, enter the cell nucleus and inhibit transcription of proinflammatory cytokines, such as interleukin-1, interleukin-2, tumour necrosis factor- α (TNF- α) and proinflammatory enzymes, including collagenase, elastase, and plasminogen activator [29].

Symptomatic management of fixed neurological deficits

Fixed neurological deficits in multiple sclerosis are best managed by a multidisciplinary team, attending to physical therapies, psychological, and social interventions supplemented by medical treatments. The benefits of intense inpatient rehabilitation outlast the duration of therapy by up to 9 months [30]. The symptoms that are most amenable to treatment are spasticity and sphincter dysfunction. Spasticity causes discomfort and hinders care and is usefully treated by baclofen, which acts on spinal cord GABA-B receptors to suppress reflex arcs that have been released from higher inhibitory control; or tizanidine, which acts through spinal cord α_2 receptors to modulate presynaptic release of excitatory aminoacids. Bladder symptoms are most easily categorised by measuring the postmicturition bladder volume. If greater than 100 mL, there is primarily failure to empty and the treatment is ideally intermittent self-catheterisation; if the bladder empties fully but stores poorly, the detrusor might be inhibited by anti-cholinergics such as oxybutynin [31]. In fact, most patients have a combination and experience the urge frequently to empty a partially filled bladder against a closed sphincter. Erectile impotence is successfully treated with sildenafil citrate, a phosphodiesterase inhibitor that acts predominantly on nitric oxide within the penile vasculature. Paroxysmal attacks respond well to membrane-stabilising drugs - typically carbamazepine. No pharmacological treatment has shown a useful effect on the tremor of multiple sclerosis. There are advocates for thalamotomy and thalamic stimulation in highly selected patients. Fatigue cannot be satisfactorily treated; lowering body temperature might help and small trials report some benefit from amantadine and modafanil [32].

Prospects for improved treatment of disease activity

In view of the fact that the ability to suppress relapses and limit their consequences is partial, no informed analyst could reasonably conclude that (despite their achievements) the β -interferons are a definitive therapy in multiple sclerosis. The pharmaceutical industry has responded by sponsoring studies with combinations of established drugs (such as β -interferon and cyclophosphamide) without compelling evidence for synergistic benefit to date, together with a significant investment in novel immunotherapeutic strategies.

There are two approaches to reduce the activation and proliferation of autoreactive T cells. One is to search for new agents that suppress immune activity non-specifically and have acceptable safety profiles. Past attempts (with cyclophosphamide, ciclosporin, lymphoid irradiation, cladribine) have shown evidence for efficacy but with major side-effects; examples of this legacy are paclitaxel, teriflunomide, and autologous bone marrow transplantation, in which the limited efficacy seen to date must be weighed against the procedural mortality of around 5% [33]. The second strategy is to assume that the specific interaction between MBP, T cells, and antigen-presenting cells is the pivotal event driving multiple sclerosis. Several drugs have been designed to manipulate this interaction - for instance, vaccination with T cell receptor subtypes [34], MBP specific T cell clones [35], or disrupted MBP peptides. Although the results were disappointing, it would be premature to judge whether the strategy is wrong or the reagents insufficiently active. The hope was that, by minor changes in the presumed immunodominant peptide, autoaggressive MBP-reactive T cells might be tolerated. Alternatively, there are treatment strategies to reduce the effect of activated T cells; by blocking their entry into the brain (with an antibody against the α -4 integrin) or by neutralising putative toxic products [36].

Prevention of disability acquired through progression

Despite several attempts, immunomodulatory drugs are of little use once axonal degeneration has reached a critical threshold and clinical progression is established [37]. It follows that there might be an opportunity, early in the disease course, to suppress those components of the inflammatory process that initiate the cascade leading to delayed progression. Thus, the aim of immunotherapies is not only to reduce relapse frequency, but also to prevent transition to the secondary progressive phase of the illness. These essential issues in the therapy of multiple sclerosis - does early effective antiinflammatory therapy reduce the proportion of patients who ever enter the secondary progressive phase, or usefully affect the slope of that progression? - are now being addressed in trial design [38].

Can surviving axons be remyelinated?

The informed patient often expresses disappointment that management aims merely to limit further damage without seeking to restore the neurological past. Endogenous remyelination is limited to the acute inflammatory phase, and this timing raises the issue of whether, paradoxically, anti-inflammatory treatment might contribute to the failure of repair. For those axons that degenerate early as a direct result of the inflammatory process, efforts at remyelination might have little to offer; conversely, if the

naked axon is resistant to the inflammatory milieu but has poor survival properties, remyelination might be neuroprotective and its timing important.

The therapeutic challenge is whether to enhance endogenous remyelination or develop exogenous cell-based therapies. Experimentally, endogenous remyelination restores conduction and function in young and adult nervous systems [39]. The lesions of multiple sclerosis do contain oligodendrocyte progenitors, but these seem unable to usefully engage naked axons [40]. Manipulation of mechanisms involved in receptor-ligand growth factor interactions during the inflammatory phase of tissue injury might energise these indolent progenitors and improve remyelination. Thus, one option is to wait until a therapy is available that can be given systemically and delivered simultaneously to all affected parts of the central nervous system. The alternative is first to prove that structure and function can usefully be restored in a single informative lesion before tackling the secondary task of making this intervention diffusely available in the central nervous system. The initial proof of principle will almost certainly involve cell implantation; at present, the most promising candidates are autologous peripheral nerve Schwann cells [41] or olfactory bulb ensheathing cells [42]. How best to plan the difficult transition from experimental to clinical science in the context of a multifocal and multiphasic disease has been much discussed. The ideal lesion would be accessible, responsible for clinically significant and stable deficits, resulting from persistent demyelination, and at a site where the risks of failure would be acceptable (perhaps through the presence of an intact paired structure or pathway) and where tissue was shown to be undergoing progressive axonal degeneration in the absence of active inflammation. The optic nerve is perhaps the best candidate, because the symptoms are clinically eloquent, physiological assessment and imaging are well developed, and serial atrophy is seen after unilateral optic neuritis despite recovery of vision [43]; this combination suggests postinflammatory axonal degeneration consistent with loss of trophic support from myelin [22].

CHALLENGES

For the pathologist, multiple sclerosis is a disorder of the central nervous system, manifesting as acute focal inflammatory demyelination and axonal loss with limited remyelination, culminating in the chronic multifocal sclerotic plaques from which the disease gets its name. For the patient, multiple sclerosis threatens an apparently infinite variety of symptoms but with certain recurring themes and an unpredictable course. For the neurologist, multiple sclerosis is a disorder of young adults diagnosed on the basis of clinical and paraclinical evidence for at least two demyelinating lesions, affecting different sites within the brain or spinal cord, separated in time. For the clinical scientist, multiple sclerosis is the prototype inflammatory autoimmune disease of the central nervous system in which knowledge gained across a range of basic and clinical neuroscience disciplines has already allowed rational strategies for treatment. For all these groups, multiple sclerosis remains a difficult disease for which solutions seem attainable yet remain elusive.

A major part of future studies will be to resolve the question of disease heterogeneity [44,45]. Because primary progressive multiple sclerosis affects an older (predominantly male) population, has a less favourable prognosis, and is associated with fewer radiological and histological inflammatory lesions - such that these patients are disenfranchised with respect to clinical trials of immunomodulatory drugs - this type of multiple sclerosis is considered by many to be a separate disorder [46]. Genetic analyses suggest specifically different MHC associations in northern Europeans and the Mediterranean (especially Sardinians), and (perhaps) between primary progressive and relapsing-remitting multiple sclerosis. This notion of heterogeneity is further developed in pathological studies with biopsy and necropsy material, in which four distinct but overlapping histological types are described. The histopathological appearances are generally similar between lesions from each patient, but the nature of necropsy or biopsy material makes it more difficult to show subtype consistency over time [45].

Within 40 years of its first depiction, the clinical and pathological details of multiple sclerosis had been adequately characterised. Over the past 120 years, ideas have consolidated on the cause and mechanisms of inflammatory demyelination and axonopathy. In the past 10 years, therapies have emerged that modestly affect the course of the illness. Current research is increasingly seen as coherent and focused on the hot topics that need to be solved to limit, repair, and prevent the damage caused by multiple sclerosis.

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PET VISUALISATION OF MICROGLIA IN MULTIPLE SCLEROSIS PATIENTS USING [¹¹C]PK11195

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ABSTRACT

Activated microglia are involved in the immune response of multiple sclerosis (MS). The peripheral benzodiazepine receptor (PBR) is expressed on microglia and upregulated after neuronal injury. [¹¹C]PK11195 is a positron emission tomography (PET) radioligand for the PBR. The objective of the present study was to investigate [¹¹C]PK11195 imaging in MS patients and its additional value over MRI concerning the immuno-pathophysiological process. Seven healthy and 22 MS subjects were included. Semiquantitative [¹¹C]PK11195 uptake values were assessed with normalisation on cortical gray matter. Uptake in Gadolinium-lesions was significantly increased compared to normal white matter. Uptake in T2-lesions was generally decreased, suggesting a PBR downregulation. However, uptake values increased whenever a clinical or MR-relapse was present, suggestive for a dynamic process with a transient PBR upregulation. During disease progression, an increase of normal-appearing white matter (NAWM) uptake was found, propagating NAWM as the possible real burden of disease. In conclusion, [¹¹C]PK11195 and PET are able to demonstrate inflammatory processes with microglial involvement in MS.

INTRODUCTION

Microglia, the brain's intrinsic macrophages, play a major role in the inflammatory process of autoimmune demyelinating diseases and particularly multiple sclerosis (MS). They initiate the immunological process in the early stages of the disease. More specifically, microglial activation in experimental allergic encephalomyelitis (EAE) and MS contributes to CNS damage through several mechanisms such as the production of proinflammatory cytokines (e.g. TNF- α), matrix metalloproteinases and free radicals, even as still ramified but activated cells (Benveniste, 1997). Indeed, by releasing myelinotoxic factors with direct injury to the oligodendrocyte-myelin unit, activated microglia stimulate this demyelinating process (Sriram and Rodriguez, 1997). Additionally, during relapses when the blood-brain barrier (BBB) opens, they are thought to act as antigen presenting cells having the capacity of activating perivascular myelin-reactive T lymphocytes by costimulatory molecules on their surface (Dangond *et al.*, 1997; Vowinckel *et al.*, 1997).

One of the characteristic features of microglia is their rapid activation in response to brain injury with a concomitant higher expression of the peripheral benzodiazepine receptor (PBR) (Banati *et al.*, 2000). Visualisation of this PBR is possible by means of radiolabeled PK11195, a selective and specific high affinity ligand, allowing as such the assessment of microglial activity and providing more specific *in vivo* information concerning the underlying histopathological features. Indeed, high resolution microautoradiography combined with immunohistochemical cell identification in MS and EAE tissue demonstrated that in focal inflammation, when the BBB is disrupted, the PBR is expressed on invading blood-borne cells such as macrophages (Banati *et al.*, 2000). However in brain lesions without direct damage to the BBB, the predominant cell type expressing PBR binding sites is the activated microglial cell (Banati *et al.*, 1997).

PK11195 has been labeled with ^{11}C for the study of the lesioned brain with positron emission tomography (PET) in various neuroinflammatory conditions like stroke, Rasmussen's encephalitis and cerebral vasculitis (Goerres *et al.*, 2001; Ramsay *et al.*, 1992). A previous feasibility study showed the value of a straightforward semiquantitative approach by means of defining an accurate confidence interval for the [^{11}C]PK11195 uptake values in controls for the eventual detection of microglial activation in acute and chronic neuroinflammatory diseases (Debruyne *et al.*, 2002).

Up till now, magnetic resonance imaging (MRI) has been widely used in MS to evaluate disease activity and to monitor clinical trials or the natural course of the disease process itself. Although MRI is of paramount value for diagnostic procedures, there remains a weak correlation between MRI parameters and disability as measured with the expanded disability status scale (EDSS). The reason for this clinoradiological paradox may be the lack of histological specificity of conventional MRI lesions and the underestimation of disease burden in the normal-appearing white matter (NAWM) and spinal cord (Barkhof and van Walderveen, 1999; Nijeholt *et al.*, 1998). The aims of the present study are, firstly, to

assess the [¹¹C]PK11195 uptake in MS patient subgroups with chronic and active white matter lesions on MRI and, secondly, to investigate the additional value of [¹¹C]PK11195 imaging over MRI concerning the immuno-pathophysiological process during the disease course in this cohort of patients with different clinical manifestations and invalidity.

PATIENTS AND METHODS**Subjects**

The study was approved by the Ethical Committee of the Ghent University Hospital and written informed consent was obtained from each subject. Seven healthy volunteers (3 males, mean age 33 ± 8 , range 23-41 yrs) and 22 out of 27 initially randomly included clinical definite and laboratory proven MS patients referring to the Poser criteria (Poser *et al.*, 1983) (mean age 43 ± 11 , range 26-64 yrs) were finally included. Demographic and clinical parameters of the MS patients are described in table 1. Four MS patients were treated with IFN- β at the time of inclusion. Thirteen patients had the relapsing-remitting type (RR) of the disease while 7 patients were secondary progressive (SP), having a continuous worsening of invalidity over a follow-up period of at least 6 months. Two patients had a primary progressive course (PP) without relapses from the very beginning of the disease. Six patients had a clinical relapse during the time of scanning, defined as the occurrence or worsening of neurological dysfunction lasting more than 24 hours. In 3 of them, corticosteroids needed to be administered after all imaging was performed. Ten patients showed Gd-enhancing lesions on the MR scan, 5 of them with a concomitant clinical relapse. One patient with the RR type of disease was scanned twice within a time interval of 4 months, the first imaging session at the time of a clinical relapse with Gd-lesions and the second session at the time of remission. The average disease duration was 9.3 ± 8.3 , range 0.3-32.7 yrs. The average EDSS was 4.0 ± 2.0 , range 1.0-7.0. To assess differences between moderate and severe impairment, patients were, for some analyses, subdivided into a low and high invalidity category (cut-off EDSS 4.0).

Age	Sex	Type	Disease duration (yrs)	EDSS	Clinical relapse	Gd-lesions	Sampled T2-lesions	Total T2-lesions
44	M	RR	2.3	3.0	no	7	4	32
37	F	RR	3.6	1.5	no	1	4	30
51	F	RR	22.7	2.5	yes	1	3	8
64	F	PP	13.7	7.0	no	-	2	9
45	F	PP	12.7	6.0	no	-	-	6
32	F	RR	3.1	3.0	no	1	3	25
45	F	RR	14.8	3.0	no	1	4	30
27	M	RR	3.8	1.0	yes	1	1	6
49	M	SP	8.8	7.0	no	-	3	33
50	F	SP	8.7	5.5	no	-	2	27
38	F	RR	0.3	1.5	yes	11	4	10
51	F	SP	23.7	4.5	no	-	2	28
36	M	RR	0.7	5.5	no	-	6	19
31	M	RR	13.2	3.5	no	-	5	41
35	F	SP	7.7	4.5	no	1	3	19
60	M	SP	32.7	6.5	no	-	6	21
64	F	SP	7.6	4.5	no	-	6	28
26	M	RR	2.2	1.5	yes	-	2	2
45	F	SP	9.7	6.5	yes	2	6	16
42	M	RR	3.1	1.0	yes	1	2	12
37	M	RR	6.9	5.5	no	-	-	5
31	F	RR	3.5	3.0	no	-	1	15

Table 1 Clinical characteristics of the MS patients.

Radiochemistry

PK11195 [1-(2-chlorophenyl)-N-methyl-N-(1-methylpropyl)-3-isoquinolinecarboxamide] was obtained from RBI (Natick, MA, USA). [^{11}C]PK11195 was synthesized according to a procedure described by Camsonne *et al.* (Camsonne *et al.*, 1984). Briefly, 3 μmol N-desmethyl PK11195 was dissolved in 150 μL dimethylsulphoxide, containing 3 μmol tetrabutylammonium hydroxide. After trapping of [^{11}C]CH₃I, the vial was closed and heated at 80°C for 3 min. Purification was done by HPLC using a RP-C18 column (Econosil, 250 mm x 10 mm, 10 μm particle size) and an ethanol/water (70/30) mixture as mobile phase. Radiochemical yield towards [^{11}C]CH₃I was 57 \pm 2 %. Finally, 3.7 GBq [^{11}C]PK11195 was obtained with a specific activity of 25 GBq/ μmol . Chemical and radiochemical purity were higher than 99%. All subjects were injected intravenously with 370 \pm 10 % MBq [^{11}C]PK11195 with a slow bolus in a time course of 30 seconds.

Data acquisition and processing

All subjects underwent MR and PET scanning on the same day.

MR imaging was performed on a 1.5 T commercial MR scanner (Siemens, Magnetom 1.5 T, SP4000; Erlangen, Germany). Prior to the administration of gadolinium (Gd), standard spin-echo imaging was carried out in 5 mm thick axial planes (pixel size=0.9 \times 0.9 mm²) with proton density- (TR/TE/NEX=2170/20/1), T2- (TR/TE/NEX=2170/80/1) and T1-weighted (TR/TE/NEX=600/12/1) contrast. Five minutes after Gd injection, the axial slices were rescanned with T1-weighting (TR/TE/NEX=800/20/1).

PET studies were performed on a Siemens ECAT 951/31 PET scanner (Siemens, Knoxville, TN, USA) with a transaxial and axial resolution (FWHM) of 5.8 and 5 mm respectively, operating in 2D mode. All subjects were placed in supine position with dimmed lights and low ambient noise. Reconstruction was done using filtered backprojection with a Hanning filter with a (cut-off 0.5 cycles/cm). Sequential transmission scanning was performed using a germanium - 68 / gallium - 68 ring source. Correction for scatter was done using the standard software provided by the manufacturer (CTI). Subsequently, regional cerebral blood flow (rCBF) images were acquired by [^{15}O]CO₂ inhalation at 900 MBq/min. For this, the steady state technique using [^{15}O]CO₂ was applied (Frackowiak *et al.*, 1980). Eight min later, a one-hour dynamic PET study was conducted following the injection of 370 MBq [^{11}C]PK11195. Nineteen frames each consisting of thirty-one planes of 3.375 mm thickness were recorded over 60 min with an increasing duration of 2 * 5 s, 5 * 10 s, 4 * 1 min, 2 * 3 min, 1 * 4 min, 1 * 5 min and 4 * 10 min. No partial volume correction was applied. Since a previous feasibility study showed that the time-activity curves for both volunteers and patients had a similar decline with a steady-state period from 40 min postinjection, data obtained from 40-60 min postinjection were summed (static scans). Automatic radioactive decay correction was applied to all images. Individual automatic coregistration of MR and perfusion PET data was achieved using SPM99 (Statistical Parametric Mapping, Functional Imaging Laboratory, Wellcome Department of Cognitive Neurology, Institute of Neurology, London, UK) (Friston *et al.*, 1991). Spatial normalisation was done on the normal templates for T1-weighted MR in MNI space (Montreal Neurological Institute), using non-linear warping with 7 \times 8 \times 7 basic functions (5 iterations), and to a voxel size of 3 \times 3 \times 3 mm³. T2-, Gd- and coregistered PET data underwent the same transformation as the original T1-image. The same spatial transformation as for the perfusion PET studies was applied to all [^{11}C]PK11195 data. Five patients were excluded because of head movement and subsequent incorrect coregistration between the perfusion and receptor PET scan.

Volumes of interest and semiquantification

Since no generally accepted model of absolute quantification of [^{11}C]PK11195 specific binding in normal brain has been widely validated, and moreover, as no dynamic data for all volunteers were available and no arterial sampling was carried out, a straightforward semiquantitative approach was performed on the static scans. Volumes of interest (VOIs, on average 400 voxels ranging from 5 to more than 3000) were manually defined on the reoriented high-resolution MR scans in white and gray matter for volunteers and NAWM, gray matter, T2- and T1-Gd-lesions for MS patients and automatically transferred onto the reoriented [^{11}C]PK11195 scans by means of PMOD, a kinetic modeling and image fusion environment tool in JAVA (Zurich, Switzerland) (Mikolajczyk *et al.*, 1998). When drawing VOIs, care was taken to avoid the carotid and major cerebral arteries as well as the ventricles and venous sinuses. For all controls, 52 VOIs were sampled in white matter and 264 in gray matter. For all MS patients, 153 VOIs were sampled in NAWM and 84 in gray matter. Gray matter was divided in cortical and central gray matter (thalamus and striatum) because higher binding of [^3H]PK11195 was described in diencephalic structures notably in several thalamic nuclei (Doble *et al.*, 1987). The normalised specific uptake for a particular VOI was defined as the mean number of counts per volume unit in this VOI divided by the mean number of counts per volume unit in cortical gray matter. Since there was a significant age difference between patients and controls, the effect of age in controls for white matter, cortical and subcortical gray matter, and thalamic [^{11}C]PK11195 uptake values was studied.

Statistical analysis

Data were analysed by means of SPSS v10.0 for Windows (Chicago, IL, USA). For normality testing, a Kolmogorov-Smirnov test statistic was applied. For differences between groups, an independent samples t or a Mann-Whitney U test was applied when appropriate. A p-value lower than 0.05 was considered as significant while a value lower than 0.10 was considered as a meaningful trend. No Bonferroni correction was performed. Data are given as means \pm one standard deviation.

RESULTS

$[^{11}\text{C}]\text{PK11195}$ uptake values for MS patients versus controls and effect of age

A $[^{11}\text{C}]\text{PK11195}$ uptake value of 100.3 ± 9.9 in white matter and 100.5 ± 9.4 in gray matter for controls was found. In patients, NAWM and gray matter uptake was respectively 101.7 ± 11.1 and 101.0 ± 9.4 , both higher, however, not statistically significant different from white and gray matter in controls ($p=0.3$ and 0.7 respectively). No effect of age was found in controls for white, cortical and subcortical gray matter, or thalamic $[^{11}\text{C}]\text{PK11195}$ uptake values. In T2-lesions, the uptake tended to be lower compared to white matter in controls (97.3 ± 13.8 , $p=0.06$). Regarding Gd-lesions, $[^{11}\text{C}]\text{PK11195}$ uptake was significantly higher ($p=0.001$) compared to normal white matter (110.9 ± 14.7). Figure 1A shows the raised $[^{11}\text{C}]\text{PK11195}$ uptake corresponding with a Gd-lesion on MRI.

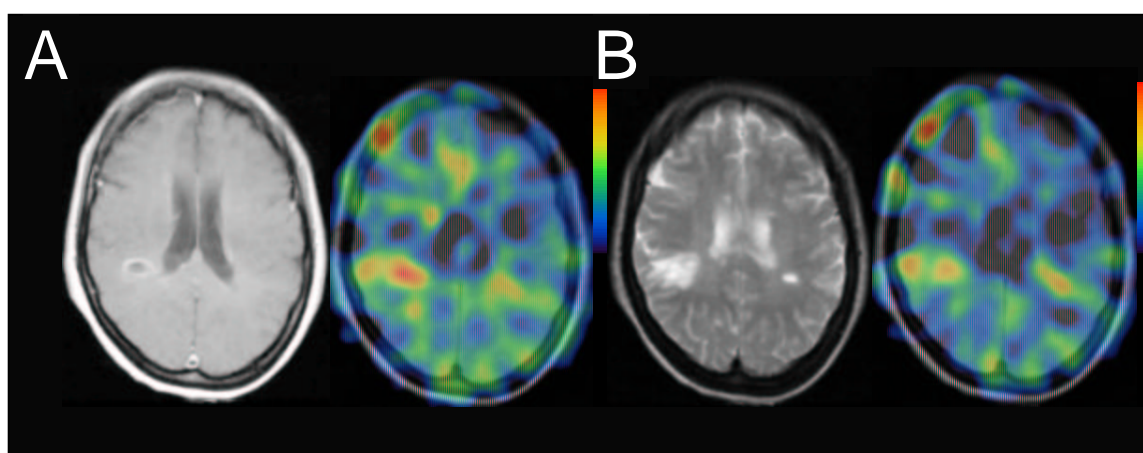


FIGURE 1: Illustration of the remote projected neuroinflammatory response in the wake of a primary lesion elsewhere. Gd-lesion located in the right periventricular parietal region in a patient with active relapsing-remitting MS with the corresponding focally increased uptake on the $[^{11}\text{C}]\text{PK11195}$ image (A). On a slightly higher level, the patient has a T2-weighted MR-lesion in the left periventricular parietal region corresponding with the concomitantly raised uptake on the $[^{11}\text{C}]\text{PK11195}$ image (B). On the same image, the increased uptake of the upper border of the Gd-lesion in the right parietal region is still visible. Note the uptake in the frontal meningeal area on both $[^{11}\text{C}]\text{PK11195}$ images, indicating the aspecific signal of $[^{11}\text{C}]\text{PK11195}$. Both $[^{11}\text{C}]\text{PK11195}$ images are superimposed on the corresponding proton density-weighted MR scan.

Figure 2 shows the mean $[^{11}\text{C}]\text{PK11195}$ normalised uptake values for different types of MRI-lesions in MS patients.

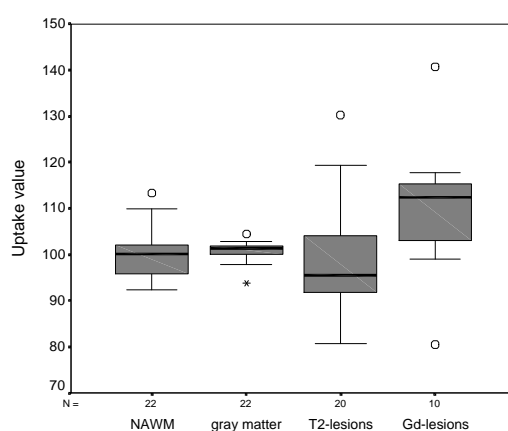


FIGURE 2: Boxplot of $[^{11}\text{C}]\text{PK11195}$ normalized uptake values in different types of MRI-lesions.

[¹¹C]PK11195 uptake values for MRI-lesions subdivided according to the presence of a relapse (clinical or MR-relapse)

A higher [¹¹C]PK11195 uptake for T2-lesions was found in patients presenting at the time of scanning with an attack, defined as a clinical relapse or the presence of Gd-lesions on MRI (100.7 ± 14.2 versus 93.7 ± 12.5 ; $p=0.01$, figure 3). Also, when subdivided according to the presence of Gd-lesions on MRI or a clinical relapse separately, [¹¹C]PK11195 uptake values were higher in both situations (respectively $p=0.05$ and 0.02). Table 2 shows the T2-lesional [¹¹C]PK11195 uptake values for the distinct conditions. The single patient with the RR type of disease, which was scanned twice, had a mean T2-lesional uptake value of 130.3, which dropped to 100.9 four months later at the time of remission. Figure 1 shows the raised [¹¹C]PK11195 uptake corresponding with a T2-lesion in a patient with the RR type of disease during a clinical and MR-relapse.

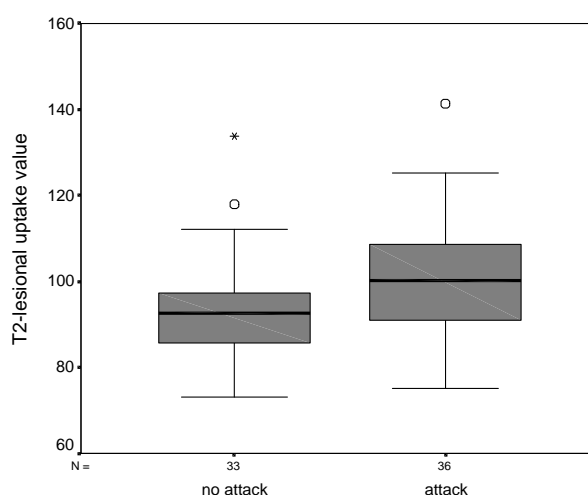


FIGURE 3: Boxplot of [¹¹C]PK11195 uptake values for all T2-lesions subdivided according to the presence of an attack (clinical or MR-relapse).

o = outlier value (cases with values between 1.5 and 3 box lengths from the upper or lower edge of the box. The box length is the interquartile range); * = extreme value (cases with values more than 3 box lengths from the upper or lower edge of the box)

	Clinical relapse	MR-relapse	Attack
present	105.0 ± 16.6	101.7 ± 13.9	100.7 ± 14.2
not present	94.6 ± 11.7	93.1 ± 12.5	93.7 ± 12.5
p-value	0.02	0.05	0.01

Table 2 [¹¹C]PK11195 uptake values for T2-lesions, subdivided according to the presence of a relapse (clinical or MR-relapse).

When the [¹¹C]PK11195 uptake for Gd-lesions was subdivided according to the coinciding presence of a clinical relapse, uptake was higher when a relapse was present (104.4 ± 17.0 versus 115.4 ± 11.3 ; $p = 0.05$).

No significantly different NAWM [^{11}C]PK11195 uptake was found when a relapse was present.

Correlation of lesional [^{11}C]PK11195 uptake values with disease duration and invalidity

Concerning the relationship between NAWM [^{11}C]PK11195 uptake values and disease duration, a steady rising slope during the progression of the disease was found ($r=0.4$; $p=0.05$; figure 4). Without the outlier value (see figure 4), the positive correlation remained, however, statistically non-significant ($p>0.1$). Concerning the correlation between gray matter [^{11}C]PK11195 uptake and disease duration, subdivided according to high and low invalidity category patients, significance was reached for the high invalidity patients only ($r=0.6$; $p=0.05$). The correlations between [^{11}C]PK11195 uptake values for both T2-weighted lesions and Gd-lesions on one side and EDSS or disease duration on the other side did not reach statistical significance.

Thalamic and NAWM [^{11}C]PK11195 uptake in PP MS patients

For the two patients with the PP type of MS, a substantially higher uptake was found both in the thalamus (mean values respectively 109.9 for PP, 104.0 for RR and 104.3 for SP; p-value of 0.3 PP versus RR) and the NAWM (mean values for all lesions respectively 104.1 for PP, 99.8 for RR and 100.7 for SP; p-value of 0.1 PP versus RR).

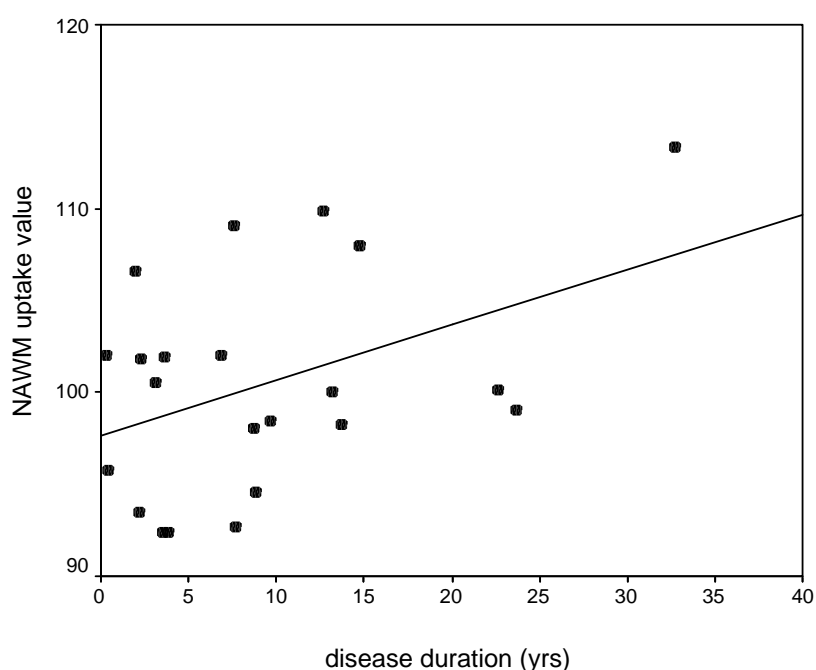


FIGURE 4: Correlation of NAWM [^{11}C]PK11195 uptake and disease duration.

DISCUSSION

Radiolabeled PK11195 has been validated as a marker of microglial proliferation, with its ensuing increased PBR density, in ample neuropathological and animal experimental work involving lesions with or without BBB damage. Moreover, the full transformation of microglia into parenchymal phagocytes, absent in areas with chronic or subtle brain pathology, is not necessary to reach maximal levels of PK11195 binding (Banati *et al.*, 1997; Benavides *et al.*, 1988). An equal observation was made in a previous study in MS patients, where a high [^{11}C]PK11195 uptake occurred in active white matter inflammation defined by MR, reflecting the presence of activated microglia (Vowinckel *et al.*, 1997). The latter findings were confirmed in the present study where significantly increased [^{11}C]PK11195 uptake values were found in patients with active focal inflammatory lesions defined by Gd-enhanced T1-MRI (figure 1 and 2). The increased uptake in Gd-lesions is in accordance with the known histology of these conventional MR lesions. Indeed, in focal Gd-enhanced T1-weighted MRI lesions, the BBB breakdown is related to an extensive inflammatory response including macrophages and T-cells (Nesbit *et al.*, 1991).

Microglia occupy 5 to 12% of the total number of cells in the normal brain. Gray matter contains more microglia than white matter, especially in sensory, limbic and subcortical gray matter structures (Lawson *et al.*, 1990). The latter was also demonstrated in a previous feasibility study where a higher mean gray matter [^{11}C]PK11195 uptake was detected in seven controls (Debruyne *et al.*, 2002). Although a larger group of MS patients of the PP type is needed to make a clearer statement, the higher thalamic [^{11}C]PK11195 uptake found in the present study could be explained by a projected neuroinflammatory response secondary to descending corticothalamic tract lesions but, alternatively, also due ascending to spinal cord long tract lesions such as in myelopathic syndromes, typically seen in this subgroup of MS patients (Andersson *et al.*, 1999; Banati *et al.*, 2000; Sorensen *et al.*, 1996). This hypothesis of a remote neuroinflammatory response in the wake of primary lesions elsewhere along a neural pathway was already formulated by Banati *et al.* where an increased thalamic [^{11}C]PK11195 uptake was found in a patient with a spinal cord MRI lesion, and also in a case of EAE where PBR expression was induced in the midbrain caused by an injured spinothalamic tract (Banati *et al.*, 2000).

T2-lesions on MRI are known for their high sensitivity but low specificity with regard to histopathology. The [^{11}C]PK11195 uptake for T2-weighted lesions in the present study was low (figure 2). As such, these findings may be related to a PBR downregulation of chronic, immunologically less triggered microglia due to the disappearance of myelin fibers, which are over time replaced by axonal scars (Johnson *et al.*, 1986; Schlumpf *et al.*, 1993; Trapp *et al.*, 1998). Then, whenever a temporarily reactivation of the autoimmune process occurs, PBR expression will be higher compared to lesions in an existing steady state, as demonstrated in the present study where an overall global T2-lesional upgrading of [^{11}C]PK11195 uptake was noticed when imaging was performed during a clinical or MR-relapse (figure 3). This upgrading of [^{11}C]PK11195 uptake is illustrated in figure 1 and was also seen in the single RR patient who was scanned twice and showed a much larger mean T2-lesional [^{11}C]PK11195 uptake value at the time of

relapse compared to the time of remission. These findings confirm earlier *in vitro* and *in vivo* observations showing activated microglia remote from the primary inflammatory site (Banati *et al.*, 2000). As such, the molecular analogue of the natural disease course in which clinical and MR relapses are followed by periods of a relative stagnation is a waxing and waning phenomenon for the PBR expression in the T2-weighted lesions.

In the present study, a slightly higher value of NAWM [^{11}C]PK11195 uptake compared to white matter of controls was found, without any significantly different radioligand uptake when a relapse was present. This is also in agreement with histopathological studies, where an increased number of MHC class II microglia attributing to a loss of myelin extending far beyond visible detectable inflammatory foci was found (Hayes *et al.*, 1987), as well as with autoradiographic studies both in EAE and human post-mortem tissue demonstrating regions of an increased number of non-phagocytic, still ramified, but activated microglia along NAWM tracts (Banati *et al.*, 2000). Also, a tendency to a rising of the NAWM [^{11}C]PK11195 uptake during disease progression was found (figure 4). These findings are in line with the hypothesis that the demyelinating process is initiated by microglia from the very beginning of the disease, unrelated to BBB disruption and autoreactive T-cell function (Kesselring, 1990), the latter being involved in clinical and MR-relapses (Miller *et al.*, 1995). As such, NAWM microglia constitutes a real burden of the disease, causing invisible demyelination independent from relapses. With this regard, Confavreux *et al.* recently concluded already that relapses do not significantly influence the progression of irreversible disability (Confavreux *et al.*, 2000).

In conclusion, with [^{11}C]PK11195 PET as a marker of the immuno-pathophysiological process, we *in vivo* raise evidence to the hypothesis that microglia may play an important role in the immunopathogenesis of multiple sclerosis. For T1-Gadolinium-weighted MR lesions, the [^{11}C]PK11195 uptake was significantly increased. Concerning T2-weighted MR lesions, the microglial activity was decreased suggesting a PBR downregulation related to the gradual vanishing of myelin fibers towards the chronic degenerative phase. An increased uptake in these lesions was found in patients with a clinical relapse or the presence of remote Gd-lesions, indicating a dynamic process with a transient upregulation following the natural course of the disease. In NAWM, the increase of [^{11}C]PK11195 uptake with disease duration is in line with the theory proposing NAWM microglia as a real burden of the disease, causing invisible demyelination independent from relapses.

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IMAGING OF MICROGLIAL ACTIVATION WITH PET AND ATROPHY WITH MRI IN MULTIPLE SCLEROSIS: INTERRELATIONSHIP AND CLINICAL CORRELATES

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ABSTRACT

Objective: The objectives of the present study were to assess brain atrophy in MS patients during different disease stages and to investigate by PET and [¹¹C]PK11195, a marker of microglial activation, the relationship between inflammation, atrophy, and clinical relevant measures.

Methods: Eight healthy subjects and 22 MS patients were included. Semiquantitative [¹¹C]PK11195 uptake values, with normalization on cortical gray matter, were measured for magnetic resonance imaging T₂- and T₁-lesions and normal appearing white matter (NAWM). As atrophy index we used the ratio of the amount of white and gray matter divided by the ventricular size, using an optimized a priori based segmentation algorithm (SPM99).

Results: Atrophy was significantly greater in MS patients compared to age-matched controls. A significant correlation was found between brain atrophy and both disease duration and disability, as measured with the expanded disability status scale (EDSS). For NAWM, [¹¹C]PK11195 uptake increased with the amount of atrophy, while T₂-lesional [¹¹C]PK11195 uptake values decreased according to increasing brain atrophy.

Conclusions: Brain atrophy, correlating with disease duration and disability, is directly related to NAWM and T₂-lesional inflammation as measured by microglial activation.

INTRODUCTION

In MS, neuroinflammation is the pivotal event that causes demyelination and oligodendrocyte cell death [1]. Whereas over the past decade most attention was focused on the theory of a T-cell mediated autoimmune process [2], *in vitro* studies however showed that microglia also can be activated by various stimuli resulting in the expression of proinflammatory cytokines, matrix metalloproteinases, and free radicals [3]. In addition, activated microglia serve as the major antigen-presenting cell in the CNS, likely contributing to aberrant immune reactivity at this site. Accordingly, it has been hypothesized that demyelination may, at least partly, be the result of microglial activation leading to the release of myelinotoxic factors that directly injure the oligodendrocyte-myelin unit [4]. As a consequence, it is believed that microglia play a prominent role in autoimmune mediated demyelinating disorders of the central nervous system.

One of the characteristic features of microglia is their rapid activation in response to brain *injury* with a concomitant higher expression of the peripheral benzodiazepine receptor (PBR) [5]. Visualization of the PBR can be performed by means of radiolabeled PK11195. This specific high-affinity ligand, allows as such the assessment of microglial activation giving more specific *in vivo* information concerning the underlying histopathological features due to neuroinflammation in general and to MS in particular [6]. PK11195 has been labeled with ^{11}C for PET and applied in various neuroinflammatory conditions like Rasmussen's encephalitis [7], cerebral vasculitis [8], and Herpes simplex encephalitis [9].

Previously, we demonstrated characteristic [^{11}C]PK11195 uptake patterns for chronic and active white matter lesions and normal appearing white matter (NAWM) in subgroups of MS patients, exemplifying an additional value of [^{11}C]PK11195 imaging over MRI concerning the assessment and monitoring of the *immuno-pathophysiological* process in MS. Moreover, a significant steady rising amount of NAWM [^{11}C]PK11195 uptake during disease progression was found, propagating NAWM as a major burden of the disease [10]. Concomitantly with the hypothesis that microglia can directly induce myelin damage through the release of proinflammatory mediators [11], this study suggested that during the disease process invisible demyelination is an increasingly ongoing NAWM process.

On the other hand, atrophy of the brain and spinal cord at postmortem examination is considered to be a hallmark of irreversible CNS damage. Indeed, MS involves substantial loss of both axonal density and volume, in addition to the well-recognized loss of myelin within lesions [12,13]. Whereas in healthy controls, the progressive loss of brain parenchyma occurs with magnitudes ranging from 0.1 to 0.3 % per year, for MS patients the reduction in brain volume is estimated at 0.4 to 5 % per year where most published patient cohorts narrow this annual loss range to 0.6 to 1 % per year [13-15], starting already in the early stage of the disease, and being associated with short-term clinical disease activity [16,17]. Although the pathologic basis of MS-related atrophy is still unclear, there seems to be a connection with the NAWM inflammatory process. As such, a rather global process, such as (MRI-)invisible demyelination with consequently a steady axonal loss might underlie this brain atrophy [18]. This was

also demonstrated by Trapp *et al.* in a postmortem study showing axonal transection as a consistent feature in NAWM [19]. Newer MR techniques, such as magnetization transfer imaging and magnetization resonance spectroscopy have confirmed this loss of brain parenchyma in the NAWM as being a major burden of disease contributing to whole brain atrophy [20,21].

The objectives of the present study were threefold: firstly, the assessment of brain atrophy in MS patients compared to age-matched normal controls, secondly, the correlation of brain atrophy with clinical measures, and thirdly, the correlation of [^{11}C]PK11195 uptake with brain atrophy measures.

PATIENTS AND METHODS

Subjects

The study was approved by the Ethical Committee of the Ghent University Hospital and written informed consent was obtained from each subject. Eight controls (3 men, five women; mean age 37.2 ± 13 , range 23-65 y) and 27 clinical definite and laboratory proven MS patients referring to the criteria of the International Panel on the Diagnosis of Multiple Sclerosis were randomly included [22]. Five patients had to be removed from the study because of head movement and subsequent coregistration errors between perfusion and receptor PET scanning. Finally, 22 patients were eligible (9 men, 13 women; mean age 42.6 ± 11 , range 26-64 y). There was no statistically significant age difference between patients and controls ($p = 0.3$). Demographic and clinical parameters of the MS patients are described in table 1. Four MS patients were treated with IFN- β at the time of inclusion. Thirteen patients had the relapsing-remitting type (RR) of the disease while 7 patients were secondary progressive (SP), having a continuous worsening of invalidity over a follow-up period of at least 6 months. Two patients had a primary progressive course (PP) without relapses from the very beginning of the disease. Six patients had a clinical relapse at the time of scanning, defined as the occurrence or worsening of neurological dysfunction lasting more than 24 hours. In 3 of them, corticosteroids needed to be administered after all imaging was performed. Ten patients showed Gd-enhancing lesions on the MRI scan, 5 of them with a concomitant clinical relapse. The average disease duration was 9.3 ± 8.3 y (range 0.3-33 y). The average expanded disability status scale (EDSS) was 4.0 ± 2.0 (range 1.0-7.0).

Age	Sex	Type	disease duration (y)	EDSS
44	M	RR	2.3	3.0
37	F	RR	3.6	1.5
51	F	RR	22.7	2.5
64	F	PP	13.7	7.0
45	F	PP	12.7	6.0
32	F	RR	3.1	3.0
45	F	RR	14.8	3.0
27	M	RR	3.8	1.0
49	M	SP	8.8	7.0
50	F	SP	8.7	5.5
38	F	RR	0.3	1.5
51	F	SP	23.7	4.5
36	M	RR	0.7	5.5
31	M	RR	13.2	3.5
35	F	SP	7.7	4.5
60	M	SP	32.7	6.5
64	F	SP	7.6	4.5
26	M	RR	2.2	1.5
45	F	SP	9.7	6.5
42	M	RR	3.1	1.0
37	M	RR	6.9	5.5
31	F	RR	3.5	3.0

RR = relapsing-remitting; SP = secondary progressive; PP = primary progressive; EDSS = expanded disability status scale

Table 1 Clinical characteristics of the MS patients

Radiochemistry

PK11195 [1-(2-chlorophenyl)-N-methyl-N-(1-methylpropyl)-3-isoquinoline carboxamide] was obtained from RBI (Natick, MA, USA). [^{11}C]PK11195 was synthesized according to a procedure described by Camsonne et al [23]. Briefly, 3 μmol N-desmethyl PK11195 was dissolved in 150 μL dimethylsulphoxide, containing 3 μmol tetrabutylammonium hydroxide. After trapping of [^{11}C]CH₃I, the vial was closed and heated at 80°C for 3 min. Purification was done by HPLC using a RP-C18 column (Econosil, 250 mm x 10 mm, 10 μm particle size) and an ethanol/water (70/30) mixture as mobile phase. Radiochemical yield towards [^{11}C]CH₃I was 57% (confidence interval 2 %, 30 experiments). Finally, 3.7 GBq [^{11}C]PK11195 was obtained with a specific activity of 25 GBq/ μmol . Chemical and radiochemical purity were higher than 99%. All subjects were injected intravenously with 370 ± 10 % MBq [^{11}C]PK11195 with a slow bolus in a time course of 30 seconds.

Data acquisition and processing

All subjects underwent MR and PET scanning on the same day.

MR imaging was performed on a 1.5 T MR scanner (Siemens, Magnetom SP4000; Erlangen, Germany). Prior to the administration of gadolinium, standard spin-echo imaging was carried out in 5 mm thick axial planes (pixel size of $0.9 \times 0.9 \text{ mm}^2$) with proton density- (TR/TE/NEX=2170/20/1), T₂- (TR/TE/NEX=2170/80/1) and T₁-weighted (TR/TE/NEX=600/12/1) contrast. Five minutes after gadolinium injection, the axial slices were rescanned with T₁-weighting (TR/TE/NEX=800/20/1).

PET studies were performed on a Siemens ECAT 951/31 PET scanner (Siemens, Knoxville, TN, USA) with a transaxial and axial resolution (FWHM) of 5.8 and 5 mm respectively (values provided by Siemens, operating in 2D mode). All subjects were placed in supine position with dimmed lights and low ambient noise. Realignment of the head to the orbitomeatal line was performed by laser guidance. Reconstruction was done using filtered backprojection with a Hanning filter (cut-off of 0.5 cycles/cm). Sequential transmission scanning was performed using a $^{68}\text{Ge}/^{68}\text{Ga}$ ring source. Correction for scatter was done using the standard software provided by the manufacturer. Subsequently, regional cerebral blood flow (rCBF) images were acquired by [^{15}O]CO₂ inhalation at 900 MBq/min. For this, the steady state technique using [^{15}O]CO₂ was applied [24]. Eight minutes later, a one-hour dynamic PET study was conducted after the injection of 370 MBq [^{11}C]PK11195. Nineteen frames, each consisting of thirty-one planes of 3.375 mm thickness, were recorded over 60 min with an increasing duration of $2 \times 5 \text{ s}$, $5 \times 10 \text{ s}$, $4 \times 1 \text{ min}$, $2 \times 3 \text{ min}$, $1 \times 4 \text{ min}$, $1 \times 5 \text{ min}$ and $4 \times 10 \text{ min}$. Automatic radioactive decay correction was applied to all images. No partial volume correction was applied. Since a previous feasibility study showed that the time-activity curves for both volunteers and patients had a similar decline with a steady-state period from 40 min post-injection, data obtained from 40-60 min post-injection were summed (static scans) [25]. Individual automatic coregistration of MR and perfusion PET data was achieved using SPM99 (Statistical Parametric Mapping, Functional Imaging Laboratory, Wellcome Department of Cognitive Neurology, Institute of Neurology, London, UK) [26]. Spatial normalization was done on the normal templates for T₁-weighted MR in MNI space (Montreal Neurological Institute), using non-linear warping with $7 \times 8 \times 7$ basic functions (5 iterations), and to a voxel size of $3 \times 3 \times 3 \text{ mm}^3$. T₂-, Gd- and coregistered PET data underwent the same transformation as the original T₁-image. The same spatial transformation parameters as for the perfusion PET studies were subsequently applied to the [^{11}C]PK11195 data.

Volumes of interest and [^{11}C]PK11195 uptake semiquantification

Since no generally accepted model of absolute quantification of [^{11}C]PK11195 specific binding in normal brain has been widely validated and no dynamic data for all volunteers were obtained neither was arterial sampling carried out, a validated semiquantitative approach was carried out on the static images obtained during the steady-state period of the [^{11}C]PK11195 brain uptake [25]. Volumes of interest (VOIs) were defined on the individual's spatially standardized high-resolution MR scan in white and gray matter for volunteers and in NAWM, gray matter, T₂- and T₁-

Gd-lesions for MS patients and automatically transferred onto the coregistered [^{11}C]PK11195 scan by means of PMOD (University Hospital Zurich, Switzerland), a kinetic modeling and image fusion environment tool in Java [27]. When drawing VOIs, care was taken to avoid the carotid and major cerebral arteries as well as the ventricles or venous sinuses. Three global regions were defined namely white matter, cortical and central gray matter (thalamus and striatum, this was done because high labeling of [^3H]PK11195 was described in diencephalic structures notably in several thalamic nuclei [28]). The normalized specific uptake for a particular area of interest was defined as the mean activity per volume unit in this area divided by the mean activity per volume unit in cortical gray matter.

Atrophy measures

Relative parenchymal fractions were assessed with the whole-brain probabilistic segmentation and volumetry module incorporated within SPM99. T_1 -weighted images were used. Since relative brain atrophy measures have shown to be superior to absolute measures for cross-sectional studies [29], images were first normalized to the MNI template using the default SPM spatial pre-processing method (normalization with bilinear interpolation, $7 \times 8 \times 7$ nonlinear basic functions, 12 iterations and medium nonlinear regularization). Then, images were segmented, without lesion extraction using the '*lots of inhomogeneity correction*' option into gray and white matter and CSF maps for which the respective volume was determined as the proportion of voxels, worked out from a subregion of the volume that encloses the brain [30]. Finally, the brain atrophy index was defined as the relative CSF volume divided by the relative white and gray matter volume. Figure one shows an image of a segmented axial MR slice of a 37-year old MS patient (panel A) and a 39-year old healthy control subject (panel B).

Statistical analysis

Data were analyzed by means of SPSS v10.0 for Windows (Chicago, IL, USA). For normality testing, a Kolmogorov-Smirnov test statistic was applied. For differences between groups, an *independent samples T test* or a *Mann-Whitney U test* was applied whereas for the correlational analysis, a Pearson or Spearman correlation coefficient was calculated, when appropriate. A *p value* lower than or equal to 0.05 was considered as significant. Data are given as means \pm one standard deviation.

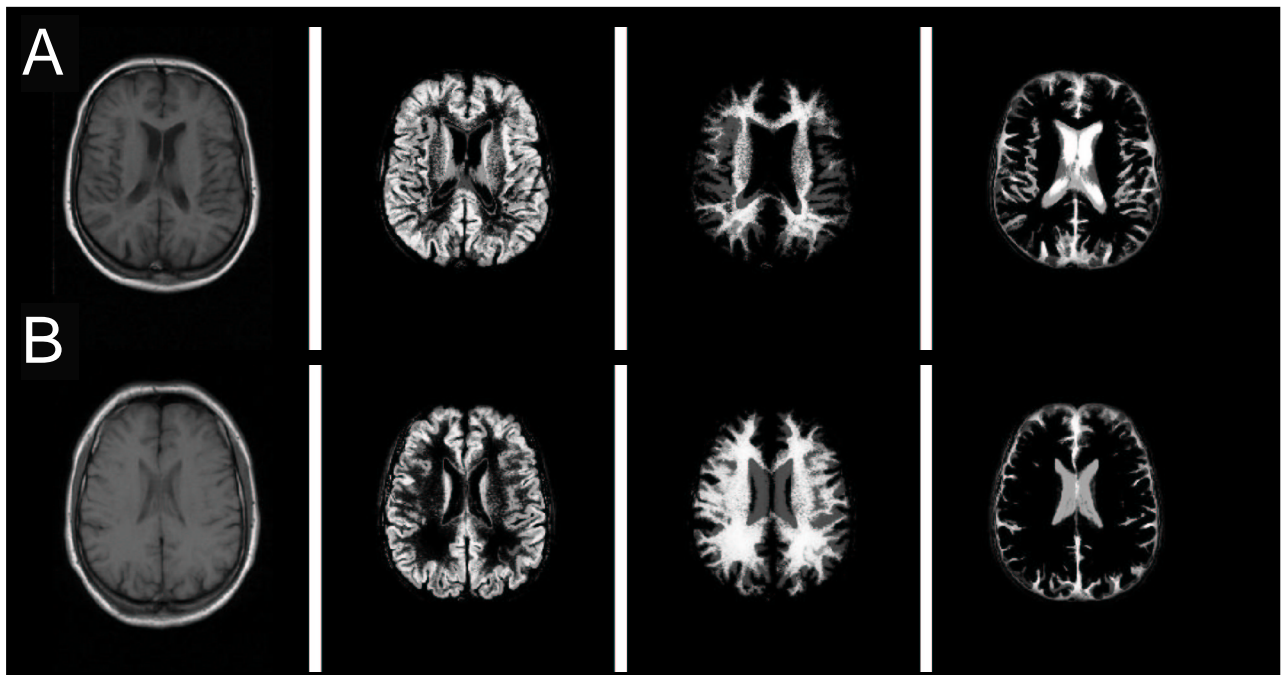


Figure 1. Example of a segmented axial MR slice into gray and white matter and cerebrospinal fluid for a 37-year old MS patient (panel A) and a 39-year old healthy control (panel B), after anatomical standardization

RESULTS

Atrophy measures for MS patients versus age-matched controls

Table 2 shows the atrophy measures for the different brain compartments. Atrophy as measured by the atrophy index was significantly greater in MS patients compared to age-matched controls ($p = 0.04$). When considering the brain compartments separately, the relative amount of gray matter, (normal appearing) white matter and CSF were all indicative of the loss of brain tissue for MS patients, however, only the difference in ventricular size (CSF) was statistically significant ($p = 0.04$). Whereas for controls a significant correlation was found between age and the amount of gray matter, CSF and the atrophy index ($p = 0.009$, $p = 0.03$ and $p = 0.02$ respectively), no statistically significant correlation was found between age and any atrophy measure for patients.

	MS patients	age-matched controls	<i>p</i> -value
<i>gray matter</i>	0.183 ± 0.011	0.186 ± 0.012	0.6
<i>(normal appearing) white matter</i>	0.102 ± 0.009	0.106 ± 0.007	0.3
<i>CSF</i>	0.089 ± 0.012	0.080 ± 0.007	0.04
<i>CSF</i> <i>gray + white</i>	0.314 ± 0.047	0.275 ± 0.034	0.04

Table 2: Atrophy comparison between MS patients and age - matched controls

Correlation of the atrophy index with disease duration and disability

As shown in figure two, there was a statistically significant correlation between disease duration and brain atrophy ($r = 0.5$; $p = 0.03$). The correlation between atrophy and disability as measured by the EDSS yielded also statistical significance ($r = 0.4$, $p = 0.05$; figure three).

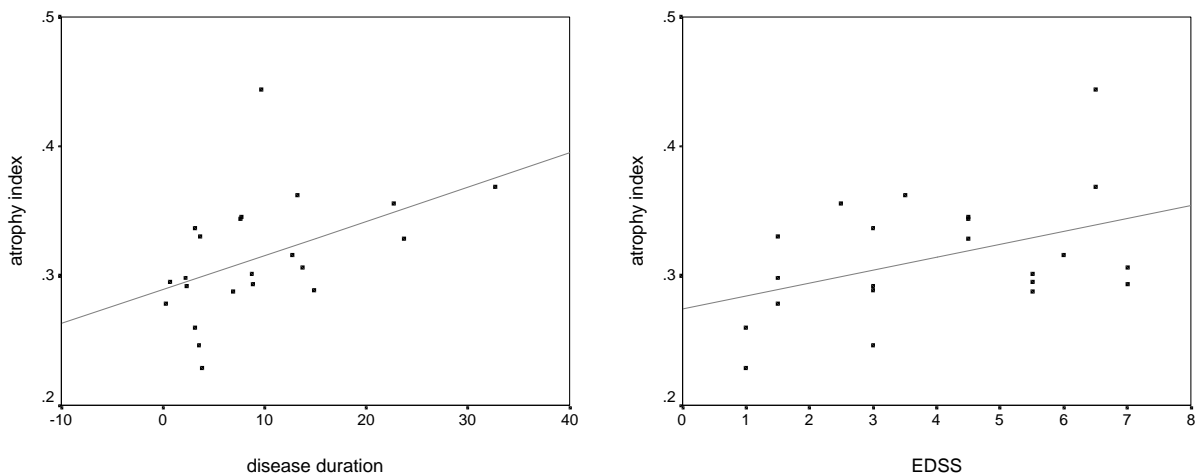


Figure 2 (left). Scatterplot of atrophy as measured by the atrophy index with disease duration (y)

Figure 3 (right). Scatterplot of atrophy as measured by the atrophy index with disability (EDSS)

Correlation of lesional [^{11}C]PK11195 uptake values with atrophy

Figure four demonstrates the relation of NAWM [^{11}C]PK11195 uptake with atrophy, indicating that the amount of NAWM microglial activation as measured with [^{11}C]PK11195 PET scanning is statistically

significant correlated to the amount of atrophy ($r = 0.2$; $p = 0.03$). It was also shown that the [^{11}C]PK11195 uptake for T_2 -lesions decreases significantly with increasing brain atrophy ($r = -0.3$, $p = 0.03$; Figure five). There was no relation between [^{11}C]PK11195 uptake in gadolinium-enhancing lesions and brain atrophy ($r = -0.01$; $p = 0.9$).

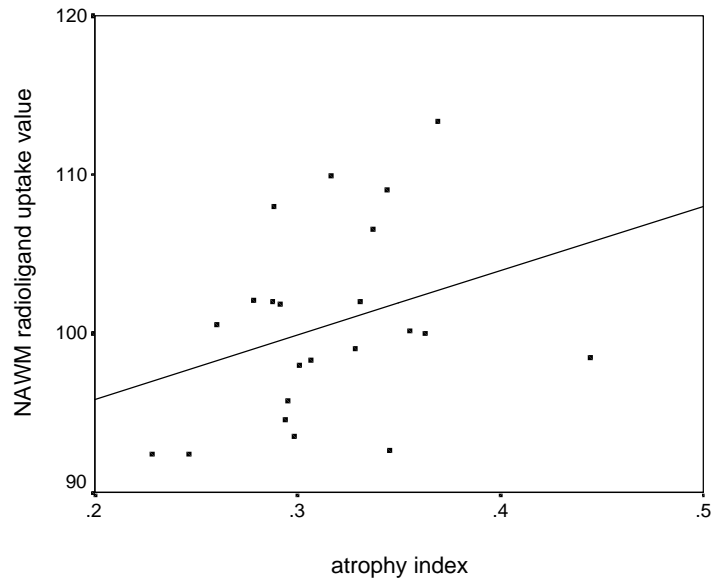


Figure 4. Scatterplot of the NAWM [^{11}C]PK11195 uptake value with atrophy as measured by the atrophy index

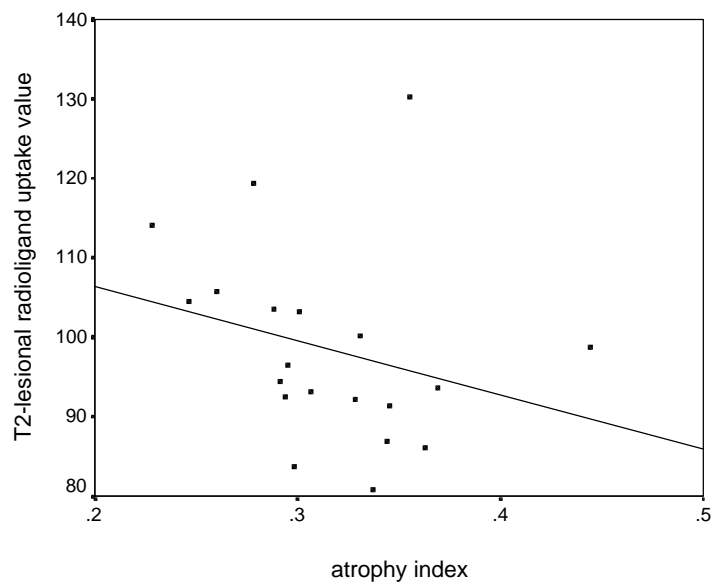


Figure 5. Scatterplot of the T_2 -lesional [^{11}C]PK11195 uptake value with atrophy as measured by the atrophy index

DISCUSSION

Recent MRI studies in MS have emphasized that brain atrophy is a robust and pivotal marker of disease progression, reflecting the destructive processes as a result of extensive axonal damage [15,16]. However, the assessment of cerebral atrophy by MRI is difficult due to general factors such as (small) inter-individual variations in head size and intracranial volume, inconsistencies in the acquisition sequence like differences in the measured voxel size or slice thickness, movement artifacts, magnetic field inhomogeneities and variations in MR image intensity scales. In addition, also disease-specific aspects like fluctuations of tissue water content such as in vasogenic edema coupled to active lesions or the administration of 'anti-inflammatory' treatment are potential sources of error [31,32]. Atrophy has been measured with MRI both by manual techniques as well as by semi-automated contour or thresholding segmentation techniques. Actual atrophy measures ranged from linear atrophy measures like the intercaudate distance, whole brain or ventricular width to absolute or relative volumes of ventricles, whole brain, hemisphere or some adherent slices, corpus callosum, or more specific brain structures like the cerebellum or brainstem [16,33-35].

Ideally however, the measurement technique should be fully reproducible, automated, accurate and very sensitive. In the present study the statistical parametric mapping software package (SPM99) was used for the assessment of brain atrophy which is a relatively robust method and requires no manual intervention [36]. SPM software uses prior spatial information from a database of normal brain images to classify voxels, according to their location and signal intensity characteristics, as gray matter, white matter or CSF and can be applied to both 2D or 3D images. This method was recently introduced by Chard *et al.* for the measurement of brain parenchymal, white and gray matter fractions in early relapsing-remitting MS patients making use of three-dimensional fast spoiled gradient recall MR scans with a slice thickness of 1.5 mm [37].

Measures of brain atrophy have been found to correlate to varying degrees with intellectual and memory dysfunction, dementia, and scores for neuropsychological tests [38,39]. Concerning the relationship between atrophy and disability, several conflicting results have been reported, most likely also enhanced by varying atrophy measures throughout different studies. The present study found a significant correlation between atrophy and disability, as measured by the EDSS, which is in agreement with most previously reported findings [40-47]. However, Wilson *et al* found no correlation between cerebral volume and clinical disability [48] while Ge *et al* as well found no significant correlation between fractional white nor gray matter volume and disability in a group of 27 RR MS patients [49].

In a previous study, we demonstrated a slightly higher NAWM [¹¹C]PK11195 uptake compared to normal white matter where the NAWM [¹¹C]PK11195 uptake showed a steady rising slope with disease progression indicating the growing amount of activated microglia, undetectable for MRI in this brain area [10]. The present study demonstrates the weak, however significant correlation between this rising NAWM [¹¹C]PK11195 uptake during disease progression and the decrease in brain parenchymal volume.

It has to be noted however that this study was not a longitudinal study but rather a snapshot study of patients with a different disease duration, making it rather difficult to draw formal conclusions about disease progression and as such necessitating extrapolations. Yet, this is the first study to reveal *in vivo* the direct relationship between NAWM inflammation or microglial activation as measured with radiolabeled PK11195 on one hand and atrophy on the other hand and demonstrates that abnormalities in the NAWM are one factor, if not one of the most important, contributing to neurological impairment [50,51]. The mechanism of neuroinflammation leading to atrophy is most probably mediated by a steady ongoing NAWM process of invisible demyelination by activated microglia. Indeed, a study by Yin *et al.* with myelin-associated glycoprotein (MAG) deficient mice demonstrated already this relationship between demyelination and atrophy where the absence of MAG led to chronic atrophy of myelinated axons and axonal degeneration [52]. This process of (hypo)myelination seems pivotal in the evolution of brain atrophy and is maintained by the lack of neurotrophic factors like MAG in the myelin sheath which are important for the protection of the cytoplasmic collar and the periaxonal space [53].

The present study did not reveal any correlation between T₁-Gadolinium-enhanced lesional [¹¹C]PK11195 uptake and brain atrophy. This is in concordance with Saindane *et al.* where the relationship between the Gadolinium-enhancing T₁ lesion load and the development of whole brain atrophy over a 2-years period was investigated and no correlation was found [18]. This suggests that the breakdown in the blood-brain barrier may be considered as an epiphenomenon in the process of brain atrophy giving rise to localized inflammation with reversible edema and some degree of focal axonal damage. Moreover, both magnetization transfer and magnetic resonance spectroscopy studies established that a rather global process underlies atrophy in MS [18,54,55], which was confirmed in the present study indicating the NAWM as a substantial contributor to brain atrophy.

The results of this study implicate the role of activated microglia in the overall demyelinating process especially in NAWM and emphasize the important long-term relationship between neuroinflammation and brain atrophy, the latter evolving by mechanisms that are at least partly independent of those mechanisms responsible for MRI lesions.

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CHAPTER SIX
RADIOLABELLED PK11195 IN ALZHEIMER'S DISEASE

**ASSESSMENT OF NEUROINFLAMMATION AND MICROGLIAL ACTIVATION IN
ALZHEIMER'S DISEASE WITH RADIOLABELLED PK11195
AND SINGLE PHOTON EMISSION COMPUTED TOMOGRAPHY: A PILOT STUDY**

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ABSTRACT

Objectives: Inflammation contributes to degeneration in Alzheimer's disease (AD), not simply as a secondary phenomenon, but primarily as a significant source of pathology. [¹²³I]iodo-PK11195 is a single photon emission computed tomography (SPECT) ligand for the peripheral benzodiazepine receptor, the latter being expressed on microglia (brain resident macrophages) and upregulated under inflammatory circumstances. The objectives were to assess AD inflammation by detecting [¹²³I]iodo-PK11195 uptake changes and investigate how uptake values relate with perfusion SPECT and neuropsychological findings. **Methods:** Ten AD and 9 control subjects were included. [¹²³I]iodo-PK11195 SPECT images were realigned into stereotactic space where binding indices, normalized on cerebellar uptake, were calculated. **Results:** The mean [¹²³I]iodo-PK11195 uptake was increased in AD compared to controls in nearly all neocortical regions, however, statistical significance was only reached in the frontal and right mesotemporal regions. Significant correlations were found between regional increased [¹²³I]iodo-PK11195 uptake and cognitive deficits. **Conclusions:** [¹²³I]iodo-PK11195 is a cellular disease activity marker and allows in vivo assessment of microglial inflammation in AD.

INTRODUCTION

Alzheimer's disease (AD), accounting for about 70% of the dementia cases is neuropathologically characterized by dense and neuritic amyloid plaques and cerebral intraneuronal neurofibrillary tangles [1,2]. However, neither plaques nor tangles correlate strongly with the degree of dementia, loss of synapses and neurons, and abnormalities of the cytoskeleton [3,4]. Over the last few years, it has become clear that inflammatory mechanisms and more specifically activated microglia, i.e. the brain resident macrophages, may contribute to the AD neurodegenerative process, not only as a purely secondary phenomenon, but also as a possible primary source of its clinical pathology [5-8]. Epidemiologically, almost 20 retrospective studies have already shown the protective effect of non-steroidal anti-inflammatory drugs (NSAIDs) in populations with a long history of NSAIDs consumption which would reduce the AD prevalence by 50% and delay its onset by 5 to 7 years [9-13]. This progression-retarding and neuroprotective effect of NSAIDs has up till now only been shown in one prospective, double-blind, placebo-controlled clinical trial of indomethacin where a significant decrease in the rate of mental deterioration in 28 AD patients was shown over a 6-months period [14]. On the other hand, other studies with diclofenac, hydroxychloroquine or nimesulide did not demonstrate this positive effect on AD progression, hence possibly indicating that influencing this neuroinflammation should be done in an early stage and maybe for a prolonged period of time [15-17].

Visualizing activated microglia and in this way inflammatory lesions in AD with positron emission tomography (PET) or single photon emission computed tomography (SPECT) would be of interest for clarifying the underlying pathophysiology, for selecting subgroups of patients that are more eligible for anti-inflammatory treatment, and, finally, for monitoring patients during trials with anti-inflammatory agents or ultimately during immunization treatment for monitoring the effective removal of amyloid deposits by activated microglia [18].

The peripheral benzodiazepine receptor (PBR) is structurally and pharmacologically distinct from the central benzodiazepine receptor (associated with GABA-regulated chloride channels), and earned his name based on his localization outside of the CNS and his high affinity for several 1,4-benzodiazepines. It is found in highest concentrations in kidneys, colon membranes, heart, steroid hormone producing cells of adrenal cortex, ovaries and testes, and several cell types of the immune system, such as mast cells and macrophages. It is also present in low concentrations throughout the brain, primarily associated with the choroid plexus, ependymal linings, and microglia [19]. Although the specific function of the PBR remains unknown, it is generally accepted to be involved in lipid metabolism and/or transport, steroid regulation, and cell proliferation [3]. The immunomodulatory role for this receptor includes the ability to modulate monocyte chemotaxis [20], cytokine expression, and to stimulate the formation of antibody-producing cells [7]. Interestingly, the PBR has the ability to reflect neuronal injury and inflammatory lesions without blood-brain barrier (BBB) damage, by an increased expression of the number of binding sites on proliferating and activated microglia, as previously indicated autoradiographically for AD [2,21].

PK11195 (1-(2-chlorophenyl)-N-(1-methyl-propyl)-3-isoquinoline carboxamide) is a specific and selective high affinity ligand for the PBR and can thus be used as a diagnostic marker for microglial activation, neuroinflammatory lesions, and finally neuronal damage. Moreover, the full transformation of microglia into parenchymal phagocytes, absent in areas with chronic or subtle brain pathology, is not necessary to reach maximal levels of PK11195 binding [22]. In vivo visualization of the human PBR, and in this way of cellular inflammatory infiltration, by means of radiolabelled PK11195 has previously been done with ^{11}C radiolabelled PK11195 for PET in various diseases like glial neoplasms, ischemic stroke, multiple sclerosis (MS), Rasmussen's encephalitis, hepatic encephalopathy, cerebral vasculitis, and herpes encephalitis [23-27]. Recently, ^{11}C -PK11195 has also been applied in early and mild dementia patients revealing an increased regional binding in the entorhinal, temporoparietal, and cingulate cortex. Moreover, serial volumetric MRI scans revealed that areas with high ^{11}C -PK11195 binding subsequently showed the highest rate of atrophy up to 12-24 months later indicating that the presence of a local immune response in cortical areas did indeed reflect an active disease process associated with tissue loss. Also, measurement of cerebral glucose metabolism revealed that areas with high ^{11}C -PK11195 binding were also characterized by decreased regional glucose use. Finally, in one patient with isolated memory impairment without dementia, the pattern of atrophy as seen by volumetric MRI imaging was predicted by the initial distribution of increased ^{11}C -PK11195 binding [28].

The application of this ligand, however, is restricted to institutions with a PET system and an in-house cyclotron that have access to these short-lived positron emitters. Therefore, the availability of a radiolabelled SPECT ligand for the study of the PBR would allow wider *clinical* application on a larger scale. Recently, we therefore assessed the biodistribution and dosimetry of ^{123}I radiolabelled PK11195 [29]. It was concluded that [^{123}I]iodo-PK11195 is a suitable and safe agent for the assessment of the PBR with a high enough specific activity required for quantitative studies [30]. The objectives of the present study were to visualize inflammation in vivo in AD patients by detecting [^{123}I]iodo-PK11195 uptake changes compared to controls and to investigate whether [^{123}I]iodo-PK11195 SPECT relates with findings obtained from perfusion SPECT and neuropsychological testing, both sensitive markers of functional brain integrity in AD [31,32,32].

PATIENTS AND METHODS

PATIENTS

The study was approved by the medical ethics committee of the Ghent University Hospital and all patients gave informed (proxy-)consent. Ten patients suffering from probable AD (4 men; mean age 77 ± 10.7 yrs (SD); range 55 to 87 yrs) according to the NINCDS-ADRDA criteria were included [33]. All had a cerebral MRI scan negative for focal lesions. As a control group, 9 normal subjects (6 men; mean age 67 ± 8.6 yrs; range 53 to 76 yrs) were included. This control group formed part of a perfusion SPECT normal database consisting of nearly 100 healthy controls, which all underwent thorough medical screening including high-resolution MRI, a complete history and physical examination, blood and urine tests, and full clinical neurological, neuropsychological, and psychiatric examination. Detailed exclusion criteria for the healthy controls are described elsewhere [34]. For ethical reasons, the AD patients' current treatment was continued during this study. Only the use of anti-inflammatory medication in general and more specifically NSAIDs for the last six months by patients and controls was an exclusion criterium for this study. Age, sex, MMSE-score, neuropsychological profile and significant perfusion defects for the AD patients are given in table 1.

Age (yrs)	Sex	MMSE	Major neuropsychological dysfunction	Perfusion defects
62.2	F	18	memory, executive, visuospatial, verbal	/
79.2	F	23	-	right frontal, right parietal
80.1	F	23	-	-
84.5	F	9	(visual) memory, executive, visuospatial	bilateral frontal, right lateral temporal, bilateral caudate head
86.5	F	14	-	left prefrontal, lateral frontal
87.3	F	25	visual	-
55.4	M	20	visuospatial	right lateral temporal, right parietal
73.3	M	23	visuospatial	left frontal
75.7	M	22	executive, visuospatial	left lateral temporal, left parietal, right frontal
85.3	M	10	memory, executive, visuospatial, verbal	right frontal, left striatum, right caudate head

Table 1 Age, sex, MMSE-score, neuropsychological profile and perfusion defects for the AD patients

METHODS

$[^{123}\text{I}]\text{IODO-PK11195}$ SPECT scan

Radionuclide synthesis and injection

^{123}I was purchased from Dupont (Dupont Pharmaceuticals Ltd., Brussels, Belgium) and PK11195 (1-(2-chlorophenyl)-N-(1-methyl-propyl)-3-isoquinoline carboxamide) was obtained from RBI (Natick, Massachusetts, USA). ^{123}I labelled PK11195 ($[^{123}\text{I}]\text{iodo-PK11195}$) was synthesized according to the method described previously [35], using a direct displacement of aromatic chlorine under solid-state conditions. The specific activity of the

labelled compound was 6.7-17.6 GBq/ μ mol (180-475 mCi/ μ mol). The total labelling yield was 50-60% and the radiochemical purity of the final product, as assessed with high performance liquid chromatography (HPLC), was more than 99%. Thyroid was blocked with Lugol's solution for all subjects (5% iodine and 10% potassium iodide; one-day protocol of 20 drops one hr before radioligand injection). The mean dose administered was 185 MBq.

Imaging and reconstruction

All subjects were scanned on a triple-headed gamma camera (Toshiba GCA-9300A, Dutoit Medical, Wijnegem, Belgium) equipped with low energy, super-high-resolution lead fan-beam collimators (measured resolution 8.1 mm) and ^{153}Gd transmission rod sources allowing transmission before emission scanning, enabling image coregistration [36]. Imaging was performed one hour after injection since stable [^{11}C]PK11195 uptake ratios were noticed as early as 20 minutes after injection reflecting pseudo-equilibrium [37]. Emission images were acquired during 20 min in a 128 \times 128 matrix with 90 projections. After triple-energy window scatter correction and uniform attenuation correction ($\mu=0.09$), images were processed by means of filtered backprojection and a Butterworth postfilter (order 8; cut-off 0.07) [38].

Estimation of binding index

After image registration into Talairach co-ordinates using a 9-parameter rigid transformation, a predefined volume of interest (VOI) analysis was performed consisting of 26 cortical, 6 subcortical, and 2 cerebellar 3D-volumes of interest for each patient (Brass, Nuclear Diagnostics, Hägersted, Sweden) [36]. Every registration with the subsequent VOI analysis was carefully checked for errors where in some cases, a manual adjustment was made when the lower cerebellar slices were not completely imaged due to subject positioning on the camera (at least five cerebellar slices had to be visualized for final inclusion). A binding index for every VOI was calculated by normalization to the cerebellum i.e. dividing the counts per volume unit in a given VOI through the counts per volume unit in the cerebellum, the latter being free of pathophysiological involvement. Comparison of binding index between patients and controls was assessed by means of a one-tailed Mann-Whitney U test since, out of neuropathological data, an increased binding index was expected for AD patients [21].

Neuropsychological testing

All patients underwent the Mini-Mental State Examination (MMSE) and a screening battery for cognitive impairment (Amsterdam dementia screening test, ADS6) containing the following subtests: picture recognition (n=8), orientation (n=8), drawing alternating sequences (n=7), verbal fluency (n=8), copying geometric figures (n=8), and free recall (n=8) [39]. Not every (sub)test could be performed in all patients due to non-compliance.

$^{99\text{m}}\text{Tc}$ -ECD perfusion SPECT scan

All patients, except for one, underwent a $^{99\text{m}}\text{Tc}$ -ECD perfusion SPECT scan. On average 30 minutes after the injection of 925 MBq $^{99\text{m}}\text{Tc}$ -ECD (ethyl cysteinate dimer; Dupont Pharmaceuticals Ltd., Brussels, Belgium). Images were acquired in a 128 \times 128 matrix with 90 projections and a frame time of 40 seconds. After triple-energy window scatter correction and uniform attenuation correction, images were processed by means of filtered backprojection and a Butterworth postfilter (order 8; cut-off 0.12). Perfusion SPECT images were automatically fitted and realigned into Talairach co-ordinates where a similar VOI analysis was performed using the same predefined VOI-map (normalization on cerebellar uptake). All patient perfusion data were averaged to assess a global group perfusion deficit. Comparison was done to 20 healthy controls (mean age 70.5 ± 6.2 yrs) [34]. For the individual patient, a hypoperfusion in a specific region was considered as significant when the uptake was less than the averaged uptake for the group of healthy volunteers minus two times the standard deviation for that specific region.

RESULTS**[¹²³I]IODO-PK11195 SPECT scan**

No effect of age was found on radiolabelled PK11195 uptake for cortical regions in controls. Grouped mean [¹²³I]iodo-PK11195 uptake values for patients and controls are shown in table 2.

		AD patients		Controls		p-value
Orbitofrontal	Left	133.8	60.6	99.2	15.4	0.04* ¹
	Right	141.9	68.6	112.8	17.8	0.2
Prefrontal	Left	143.9	55.8	100.8	20.3	0.02*
	Right	139.4	62.6	102.0	21.3	0.02*
Lateral frontal	Left	126.7	32.6	101.1	17.7	0.02*
	Right	125.7	42.9	97.7	16.4	0.03*
Superior frontal	Left	115.5	32.0	97.4	12.4	0.1
	Right	110.1	32.8	92.2	14.3	0.1
Cingulate gyri	Anterior	90.7	17.1	94.0	13.1	0.3
	Posterior	93.3	10.7	101.0	15.1	0.1
Sensorimotor	Left	109.2	41.5	106.1	14.4	1
	Right	94.4	30.4	100.6	12.1	0.2
Temporal anterior	Left	123.5	61.7	109.8	18.7	0.3
	Right	146.4	80.8	110.8	21.1	0.3
Temporal superior	Left	97.7	9.0	99.3	10.9	0.3
	Right	93.8	12.1	94.1	13.2	0.3
Temporal medial inferior	Left	106.2	15.7	99.6	11.9	0.1
	Right	103.6	28.9	92.8	12.2	0.2
Mesotemporal	Left	102.9	37.6	101.5	15.4	0.3
	Right	117.7	31.6	98.5	15.3	0.05*
Parietal inferior	Left	115.9	34.8	102.8	13.8	0.2
	Right	93.6	31.8	97.6	18.4	0.3
Parietal superior	Left	118.8	60.3	102.3	21.4	0.4
	Right	119.3	54.7	104.6	17.4	1
Occipital	Left	102.0	16.4	103.5	15.8	0.4
	Right	102.3	12.1	99.9	10.2	0.3
Basal ganglia		77.4	11.7	88.7	9.3	0.02

¹ p-values indicating significantly raised uptake values

Table 2. [¹²³I]iodo-PK11195 regional uptake values and standard deviation for AD patients compared to controls.

Elevated mean uptake values for AD patients were found in all frontal regions, temporal anterior, temporal medial inferior and mesotemporal region, left parietal inferior and parietal superior region, left sensorimotor cortex, and the right occipital region. Grouped mean [^{123}I]iodo-PK11195 uptake values for AD patients and controls are displayed in figure 1. Significantly increased uptake values were reached in the left orbitofrontal, bilateral prefrontal and lateral frontal region, and the right mesotemporal region (one-tailed Mann-Whitney U test). Figure 2 shows the [^{123}I]iodo-PK11195 uptake values for the left prefrontal and the right mesotemporal area.

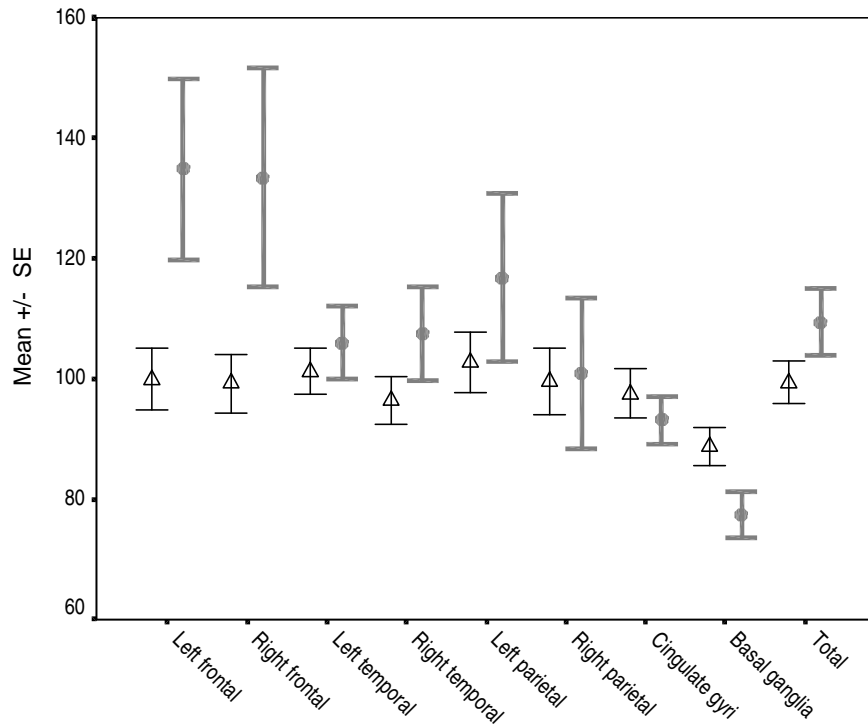


Figure 1. Grouped mean (+/- standard error of the mean) [^{123}I]iodo-PK11195 uptake values
 Δ controls; \bullet AD patients

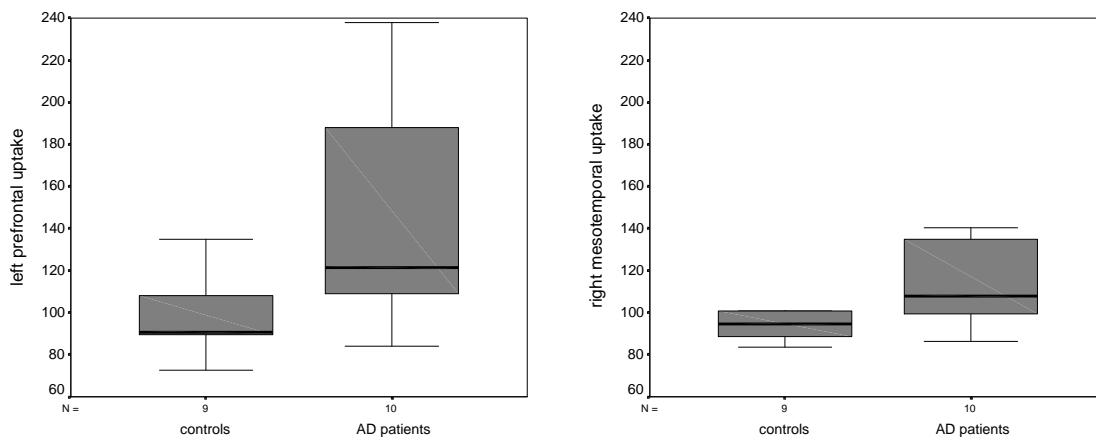
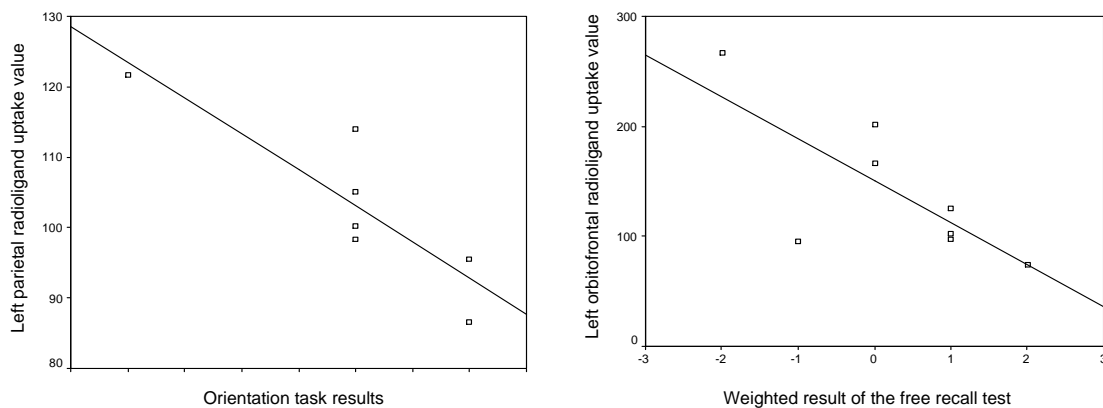


Figure 2. Boxplot of the [^{123}I]iodo-PK11195 uptake values for the left prefrontal (left) and the right mesotemporal area (right)

Neuropsychological testing and correlation with [¹²³I]iodo-PK11195 uptake values

The mean MMSE score of the AD patients was 19 ± 6 (range 9-25). Results from the picture recognition task correlated inversely with the [¹²³I]iodo-PK11195 uptake value in the right superior frontal region (two-tailed Spearman's correlation coefficient, $p=0.005$). Results of the orientation task correlated inversely with the left lateral frontal, right superior frontal and the left parietal (figure 3, left) [¹²³I]iodo-PK11195 uptake values (two-tailed Spearman's correlation coefficient, $p=0.03$, 0.04 , and 0.006 respectively). Verbal fluency results correlated inversely with the left parietal inferior [¹²³I]iodo-PK11195 uptake value (two-tailed Spearman's correlation coefficient, $p=0.007$). Results of the free recall task correlated inversely with [¹²³I]iodo-PK11195 uptake values in the left and right frontal (figure 3, right), left temporal, and the left parietal superior region (two-tailed Pearson correlation coefficient, $p=0.02$, 0.03 , 0.03 , and 0.01 respectively). No correlations were found between [¹²³I]iodo-PK11195 uptake values and the neuropsychological test results of the controls.



Inverse correlation between results of the orientation task with the left parietal [¹²³I]iodo-PK11195 uptake value (left, Spearman's correlation coefficient -0.896 , $p=0.006$) and the free recall test with the left orbitofrontal [¹²³I]iodo-PK11195 uptake value (right, Pearson correlation coefficient -0.742 ; $p=0.03$)

^{99m}Tc-ECD SPECT scan

Group perfusion defects were found in the bilateral frontal, temporal and parietal inferior regions, basal ganglia and the cingulate gyri (Independent samples t-test, $p < 0.01$, < 0.03 , < 0.02 , < 0.01 , and 0.001 respectively).

DISCUSSION

The present study describes the in vivo assessment of activated microglia in AD using radiolabelled PK11195 and SPECT. As such, this is the first SPECT study to show inflammatory lesions in AD and hence may be a potential parameter for investigational studies or therapeutic trials aiming for the inflammatory component. A previous PET study did not show an increased ^{11}C PK11195 uptake in a series of 8 AD patients [40]. However, the use of only one normal elderly subject together with glioma patients as controls could have hampered this analysis. On the other hand, the present findings are in line with more recent findings with PET and ^{11}C -PK11195 in early and mild dementia patients revealing increased regional binding in the entorhinal, temporoparietal, and cingulate cortex [28]. The discrepancy between these two studies however could be due the use of ^{123}I in the present study with its higher lipophilicity facilitating brain uptake influencing both specific binding and tracer kinetics [41].

With regard to regional uptake values, the fact that mean [^{123}I]iodo-PK11195 uptake values are increased in various regions probably indicates a widespread and diffuse inflammatory process. Likewise, increased ^{11}C PK11195 signals were found well beyond focal lesions in multiple sclerosis patients, supporting the notion that additional mechanisms apart from the focal macrophage accumulations found in the areas of BBB leakage must contribute to disease progression [25]. Moreover, the concordance between raised [^{123}I]iodo-PK11195 uptake values and perfusion deficits in frontal regions together with the significant inverse correlation between [^{123}I]iodo-PK11195 uptake values and several neuropsychological test results support the *bystander lysis* theory where activated microglia contribute to neuronal lysis by direct cytotoxic actions of some of their mediators.

Although mean uptake values were increased in various neocortical regions pathognomonically compromised in AD, significance was particularly reached in frontal neocortical regions. Although somewhat unexpected, this is in concordance with a very recent study where an intense immunoreactivity for the immune and inflammatory mediator CD40L, expressed on microglia and involved in microglia-dependent neuron death, was found throughout the frontal cortex of AD patients [8,42]. Also, this frontal increase in [^{123}I]iodo-PK11195 uptake could possibly indicate the progression together with the spreading of active inflammation towards more frontal regions in patients already at an advanced stage of the disease, although the mean MMSE score in the present study was still at a moderate level of 19. This advanced *neuropathological* stage is in concordance with the frontal perfusion deficits observed in the present study, typically seen later in the course of the disease [43]. Concerning this progression towards more frontal regions, also recent biopsy results showed that the progressive neurological impairment in AD is accompanied by a significant increase in senile plaques, neurofibrillary tangles and microglial cell activation in the frontal cortex [44]. However, group analyses should be carefully interpreted since there is a marked heterogeneity in AD patients concerning stage of the disease, progression pattern, predominant topographical lesion and cognitive subtype, with a substantial overlap between AD and other neurodegenerative conditions [43,45,46]. This heterogeneity, to which we actually contributed due to the rather large range of MMSE-score for the included AD patients, is also reflected in the larger standard deviations of [^{123}I]iodo-PK11195 uptake

values in AD patients compared to controls. Concerning this heterogeneity, behavioural as well as cognitive variability has been correlated with PET and SPECT findings [47]. Two subgroups with distinct progression rates were already distinguished segregated by neuropsychological and cerebral metabolic profiles where one rapidly deteriorating group had a significantly greater impairment in executive functions attributed to the frontal lobe and a concomitant greater frontal hypometabolism revealed by PET scanning [48].

Where the age difference between AD patients and controls could explain at least some of the perfusion SPECT findings, it cannot explain the increased [^{123}I]iodo-PK11195 uptake in AD patients since age-related increases in ^{11}C PK11195 uptake only have been described in the thalamus and no age-related effect at all was found in the present study [49]. Moreover, this age discrepancy between AD patients and controls probably made us underestimate the actual [^{123}I]iodo-PK11195 uptake due to the fact that for the current measurement no atrophy correction was performed while atrophy will be more present in the older AD group (next to the atrophy already present pathognomonically), giving rise to a loss of signal. This can be seen for example on one hand in the decreased basal ganglia radioligand uptake but also on the other hand in the lack a significantly increased radioligand uptake in the left mesotemporal region since this area, encompassing the hippocampus, is known for its substantial atrophy in AD [50].

In the present study, a semiquantitative analysis was performed with a regional normalization and the cerebellum as reference region and thus normalization factor. A regional rather than a global normalization (with whole brain as normalization factor) was preferred since a region-specific normalization is known to be more sensitive for diseases with various regions pathophysiologically involved, like AD [51]. Although some reports described the pathological involvement of the cerebellum in AD [52], this region was chosen as the normalization region since its taken together low pathologic susceptibility and the absence or at least minimal presence of upregulated inflammatory mediators in the cerebellum [53]. A previous study concluded already that the cerebellum is the more appropriate choice of reference region in the quantification of perfusion SPECT in primary degenerative dementia [54]. With regard to perfusion SPECT imaging, the cerebellum was shown to be scintigraphically uninvolved [55].

In conclusion, [^{123}I]iodo-PK11195 provides a cellular marker of disease activity (progression), able to indicate inflammatory pathology in AD patients. Interestingly, the combination of perfusion *defects* and *increased* [^{123}I]iodo-PK11195 uptake values could be able to discriminate AD patients from controls or other dementia patients, although for diagnostic purposes additional information concerning for example the test-retest reliability of [^{123}I]iodo-PK11195 SPECT scanning should be assessed. Also, the marked heterogeneity in regional increased uptake values and the concomitant large standard deviations for the different neocortical regions could probably hamper the (diagnostic) use of the present radioligand for individual patient studies. Finally, it is at present not known whether [^{123}I]iodo-PK11195 SPECT would be able to detect pathological changes in a preclinical or a very early

stage of the disease. Worthy of note is the fact that, since the PBR also has an immunomodulatory role and, moreover, PK11195 appears to possess anti-inflammatory properties [56-58], the PBR may be itself a target for therapeutic intervention. This broadens the applicability of this radioligand for the monitoring of anti-inflammatory drug treatment trials in neurodegenerative diseases.

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CHAPTER SEVEN

ROLE AND DISTRIBUTION OF SEROTONIN TYPE 2A RECEPTORS IN ALZHEIMER'S DISEASE

ROLE OF SEROTONIN AND SEROTONIN TYPE 2A RECEPTORS IN ALZHEIMER'S DISEASE

INTRODUCTION

Serotonin or 5-hydroxytryptamine (5-HT) is widely distributed in the whole brain and each receptor subtype has a specific regional distribution. It plays a role in a great variety of behaviours such as activity rhythms, food intake, sexual behaviour and emotional states. Serotonin type 2A (5-HT_{2A}, formerly called 5-HT₂) receptors, with a mainly cortical distribution, have been implicated in several largely 'neuroexcitatory' brain functions, such as appetite control, thermoregulation and sleep and play an important role in the pathophysiology of mood and anxiety disorders, schizophrenia, ageing and also Alzheimer's disease (AD). The following part explains the potential role of serotonin and serotonin type 2A receptors in Alzheimer's disease.

ROLE OF SEROTONIN AND SEROTONIN TYPE 2A RECEPTORS IN COGNITIVE BEHAVIOUR

Alzheimer's disease is typically characterised by a progressive memory impairment, predominantly a loss of short-term memory [5]. The 5-HT receptor is involved in various cognitive functions, especially learning, (working) memory and attentional processes [1]. These functions are not independent from each other or from other behavioural levels. For example, there are some connections between anxiety and memory, or between memory and attentional processes so 5-HT may modulate learning and memory by both direct and indirect ways [4]. Concerning the receptor subtypes, evidence exists that 5-HT_{2A/2C} agonists prevent memory impairment and facilitate learning (consolidation) in situations involving a high cognitive demand [4,7]. The 5-HT_{2A} receptor is thought to mediate also attentional rather than memory processes and acts by stimulating phospholipase C [3]. Finally, several interactions exist between the serotonergic and other neurotransmitter systems involved in memory. One of these interactions, especially for spatial memory, is the interaction between and modulation of the cholinergic system where 5-HT regulates the central cholinergic activity by modulating hippocampal and neocortical acetylcholine release, this through substance P interneurons. Also, the serotonergic role in learning and memory is made possible by interacting with the glutamatergic, dopaminergic or GABAergic systems [6].

ROLE OF SEROTONIN AND SEROTONIN TYPE 2A RECEPTORS IN NON-COGNITIVE BEHAVIOUR

Probably the most important role of the serotonin receptor lies in the non-cognitive aspects of Alzheimer's disease. Indeed, serotonin plays an important role in a great variety of behaviours such as food intake, activity rhythms, sexual behaviour and emotional states. After all, in many cases these non-cognitive features of AD are the main reason for hospitalisation and cause the greatest distress to caregivers. For example, 5-HT_{2A} receptor polymorphisms have been associated with both visual and auditory hallucinations and prominent psychotic symptoms [8,11].

ROLE OF SEROTONIN AND SEROTONIN TYPE 2A RECEPTORS IN AMYLOID FORMATION

Alzheimer's disease amyloid consists of amyloid β -peptides (A β) derived from the larger precursor amyloid precursor protein (APP). Non-amyloidogenic APP processing involves regulated cleavage within the A β domain followed by secretion of the ectodomain (APPs). Both the synthesis of the

amyloid precursor protein (APP) and its processing (i.e. to amyloidogenic A β peptides, soluble non-amyloidogenic APPs, and other APP fragments) are regulated by neurotransmitters. As such APP secretion is influenced by norepinephrine, prostaglandins, and muscarinic acetylcholine receptors [9]. However, the 5-HT_{2A} receptor has been suggested to regulate in a dose-dependent way APPs secretion, which could eventually lead to the formation of amyloidogenic derivatives [12].

IMMUNOLOGICAL ROLE OF SEROTONIN AND SEROTONIN TYPE 2A RECEPTORS IN ALZHEIMER'S DISEASE

5-HT has also a role in natural immunity in general, and more specifically in the superoxide production, phagocytosis, and the optimal accessory cell function of macrophages for natural killer and T-cells, which could eventually influence the removal of amyloid plaques [10]. Finally, the cerebral availability of plasma tryptophan, the precursor of 5-HT, decreases with activation of the immune system, the latter believed to be upregulated in AD [2]

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**IMAGING OF THE 5-HT_{2A} SYSTEM:
AGE-, GENDER-, AND ALZHEIMER'S DISEASE-RELATED FINDINGS**

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ABSTRACT

Serotonin (5-HT) and more specifically the 5-HT_{2A} receptor is involved in cognitive and non-cognitive behavior and plays an important role in Alzheimer's disease (AD). The objective was to assess the 5-HT_{2A} binding potential (BP) in healthy volunteers and AD with SPECT and ¹²³I-5-I-R91150, a selective radio-iodinated 5-HT_{2A} receptor antagonist. Twenty-six controls and 9 AD patients were included. A semiquantitative analysis with normalization on cerebellar uptake provided estimates of BP for 26 cortical regions of interest. An age-related decline of neocortical BP was found (11.6 % per decade). Compared to age-matched controls, a generally decreased neocortical BP in AD was found with a significant regional reduction in the orbitofrontal, prefrontal, lateral frontal, cingulate, sensorimotor, parietal inferior, and occipital region. These results are in line with previous postmortem, in vitro, and PET findings. The age-related decline highlights the necessity for matched advanced age study samples. The fact that the 5-HT_{2A} receptor is differentially affected in AD patients has implications for both the etiological basis and therapeutic management of AD.

INTRODUCTION

Approximately 90% of the total body amount of serotonin (5-HT) acts in the gastrointestinal system. Only 1-2% is present in the central nervous system where 5-HT receptors are generally involved in sleep, pain, behavior, learning, and memory [5,10]. More specifically, serotonin type 2A (5-HT_{2A}) receptors have been implicated in several brain functions, such as appetite control, sexuality, thermoregulation, and sustained attention and play an important role in the pathophysiology of mood, depressive, anxiety, and psychotic disorders, schizophrenia, ageing and also Alzheimer's disease [2,5,9,18,30,31,42].

Alzheimer's disease (AD), the most common form of dementia, is typically characterized by progressive impairment of recent memory. However, in the course of AD, other cognitive dysfunctions, behavioral and psychiatric symptoms emerge and become at least equally important [21]. The role of the 5-HT_(2A) receptor in AD is manifold. Firstly, the 5-HT_{2A} receptor has been suggested to play a role in the amyloid precursor protein secretion. Since this is linked to the β -amyloid fibrillogenesis, this could eventually lead to the subsequent formation of amyloid plaques, typically seen in AD [24,25,35,36]. Secondly, several genetic associations between 5-HT_{2A} receptor polymorphisms and the AD symptomatology e.g. visual or auditory hallucinations have been reported [23,34]. Thirdly, 5-HT has a role in natural immunity in general, and more specifically in the superoxide production, phagocytosis, and the optimal accessory cell function of macrophages for natural killer and T-cells, which could eventually influence the removal of amyloid plaques [32]. Moreover, the cerebral availability of plasma tryptophan, the precursor of 5-HT, decreases with activation of the immune system, the latter believed to be upregulated in AD [1,8]. Finally, a decrease in serotonergic cells in the central nervous system could eventually lead to a disturbance of functional interactions between the serotonergic on one hand and the cholinergic or dopaminergic system on the other hand [16,19,40,44].

¹²³I radiolabeled R91150 is a radio-iodinated 5-HT_{2A} receptor antagonist with high affinity ($K_D = 0.11 \pm 0.01$ nM). The selectivity of this ligand for 5-HT_{2A} receptors as compared to other neurotransmitter receptor binding sites such as 5-HT_{1A}, 5-HT_{1B}, 5-HT_{1D}, 5-HT_{2C}, 5-HT₃, dopamine D₂ receptors, α_1 and α_2 adrenoreceptors and histamine H₁ receptors, is at least a factor of 50. ¹²³I-5-I-R91150 binding is saturable and displaceable with the known 5-HT_{2A} receptor antagonist ketanserin and proved suitable for the imaging of 5-HT_{2A} receptors with single photon emission computed tomography (SPECT) in the human brain [11].

The objectives of the present study were, firstly, to study the age and gender effect of the 5-HT_{2A} receptor binding potential in a large group of healthy subjects (n=26) with an age range of 22 to 85 years and, secondly, to determine whether there are abnormalities in the 5-HT_{2A} receptor binding potential in AD patients compared to age-matched healthy controls, and if so, whether these abnormalities are correlated with cognitive defects or depressive symptomatology.

METHODS

PATIENTS

The study was approved by the medical ethics committee of the Ghent University Hospital and all patients gave informed (proxy-)consent. Nine AD patients (two males, mean age 81 ± 6 yrs, range 73-88 yrs) according to the NINCDS-ADRDA criteria were included with the diagnosis made by a board-certified neurologist [27]. The diagnosis was supported by the fact that there was evidence of cerebral atrophy on computed tomography or magnetic resonance imaging in all AD patients and by the fact that structural imaging did not reveal any brain disease causing dementia other than Alzheimer's disease. The control group consisted of 26 healthy subjects (11 males; mean age 51 ± 24 yrs; range 22-85 yrs). For the comparison with the AD patient group, only the oldest age group was used consisting of 9 healthy subjects (3 males; mean age 77 ± 5 yrs, range 70-85 yrs). These two groups did neither differ significantly concerning age (*Mann-Whitney U test*, $p = 0.16$) or sex (Pearson Chi-Square test, $p = 0.6$).

METHODS

¹²³I-5-I-R91150 SPECT

Radionuclide synthesis and injection

Na¹²³I was purchased from Bristol-Myers Squibb Pharma Belgium N.V. formerly Dupont Pharmaceuticals Ltd. (Brussels, Belgium). R91150 (4-amino-N-[1-[3-(4-fluorophenoxy)propyl]4-methyl-4-piperidiny] 5-iodo-2-methoxybenzamide) is an original product of Janssen Pharmaceutica (Beerse, Belgium). ¹²³I-5-I-R91150 was synthesized by electrophilic substitution on the 5-position of the methoxybenzamide group of R91150, followed by purification with high-performance liquid chromatography. The specific activity of the labeled compound was 370 GBq/ μ mol while the radiochemical purity of the final product yielded more than 99%. Thyroid was blocked with Lugol's solution for all subjects (5% iodine and 10% potassium iodide; one-day protocol of 20 drops one hr before radioligand injection). The administered dose was 185 MBq.

Image acquisition and reconstruction

All subjects were scanned on a triple-headed gamma camera (Toshiba GCA9300A, Dutoit Medical, Wijnegem, Belgium) equipped with low-energy super-high-resolution lead fan-beam collimators (measured resolution 8.1 mm) and ¹⁵³Gd transmission rod sources allowing transmission scanning prior to emission scanning, enabling image coregistration [46]. Since previously published work with sequential dynamic brain scans has shown that the cortico-cerebellar ratio reaches pseudo-equilibrium between 90 and 110 min postinjection and remains stable thereafter for up to 4 h, acquisition was started between 110 and 140 min after tracer injection [11]. Emission images were acquired in a 128 \times 128 matrix with 90 projections during 40 min consisting of 4 sequential frames of 10 min in order to omit frames when the subject was unable to complete the whole imaging session (at least two frames required for high enough count statistics). After triple-energy window scatter correction and uniform attenuation correction ($\mu=0.09$ cm⁻¹), images were processed by means of filtered backprojection and a post-reconstruction Butterworth filter of order 8 and a cut-off frequency of 0.08 cycles/cm [47].

Estimation of binding potential

After image registration into Talairach space, a volume of interest (VOI) analysis was performed making use of a predefined in-house modified VOI-map sampling the whole brain and consisting of 26 cortical, 6 subcortical, 2 cerebellar, and one pons 3D-volumes of interest (Brass, Nuclear Diagnostics, Hägersted, Sweden) [46]. Every registration with the subsequent VOI analysis was carefully checked for errors. In two subjects, a manual adjustment was necessary where the lower cerebellar slices were not completely imaged due to subject positioning on the camera (at least five cerebellar slices had to be visualized for final inclusion). The binding potential for a specific region was defined as the activity per volume element in that specific region divided through the activity per volume element in the cerebellum (void of 5-HT_{2A} receptors), expressed as a percentage. The neocortical binding potential was defined as the unweighted average of the binding potential of frontal, temporal, parietal, and occipital regions. For the comparison of AD patients to healthy controls, the binding potential values for symmetrical regions were summed to achieve improved statistics in the relatively small sample under study. An asymmetry index (AI) was calculated, defined as $AI = (R-L)/(R+L)*200$ (%).

Psychiatric and neuropsychological testing

All AD patients, except one, underwent a screening for depressive symptomatology by means of the geriatric depression scale (GDS), a reliable and validated self-rating 30 items depression screening scale for elderly populations with scores ranging from 0 to 30 with a cut-off of 9 for mild and 19 for severe depression [50,51]. Also, AD patients underwent a Mini-Mental State Examination (MMSE), a method for grading the cognitive state consisting of a series of short subtests designed to elicit information about orientation, registration, attention and calculation ability, recall, language, and praxis. It has a total score ranging from 0 to 30 with 30 representing perfect performance, with a generally accepted cut-off of 27 for the exclusion of mental impairment and 23 to 24 for the diagnosis of dementia [17,20]. Finally all AD patients underwent a screening battery for cognitive impairment (Amsterdam dementia screening test, ADS6) containing the following subtests: picture recognition (n=8), orientation (n=8), drawing alternating sequences (n=8), verbal fluency (n=8), copying geometric figures (n=7), and free recall (n=7) [14]. Not every (sub)test could be performed in all patients due to non-compliance.

Statistical analysis

Data were analyzed by means of SPSS v10.0 for Windows (Chicago, IL, USA). For normality testing, a Kolmogorov-Smirnov test statistic was applied. For differences between groups, a two-tailed *independent samples t test* or a *Mann-Whitney U test* was applied when appropriate. A p-value lower than 0.05 was considered as significant. Data are given as means \pm one standard deviation.

RESULTS

Age, sex, GDS, MMSE-score, and cognitive deficits of the AD patients are presented in Table 1.

Age	Sex	GDS	MMSE	Most prominent cognitive defects
81	F	-	-	memory
88	F	2	9	memory, orientation, attention, visuoconstruction
76	F	9	15	(visual) memory, orientation
78	F	9	21	(visual) memory
73	F	7	25	verbal memory and attention, visuospatial aspect, orientation
86	M	9	9	orientation, visuoconstruction, memory, word fluency, learning
85	F	15	20	memory, understanding, orientation
85	M	3	25	orientation, memory
74	F	19	17	visuoconstruction, language, visual memory

Table 1 Demographic variables of the AD patient group

¹²³I-5-I-R91150 SPECT uptake values

THE DISTRIBUTION OF RADIOLIGAND UPTAKE IN HEALTHY CONTROLS

The distribution of radioligand uptake throughout the brain as measured in 26 healthy volunteers is shown in figure 1. Relative regional specific uptakes compared to the cerebellum varied between 174 for the occipital cortex and 160 for the sensorimotor area. As for asymmetries in radioligand uptake, two statistically significant asymmetries were found consisting of a 2% asymmetry in frontal uptake in favor of the right side ($p = 0.003$) with the greatest difference in the prefrontal cortex (3%; $p = 0.001$) and another 3% asymmetry in favor of the left side for the temporal cortex ($p = 0.002$), with the greatest difference in the temporal superior cortex (5%; $p < 0.001$).

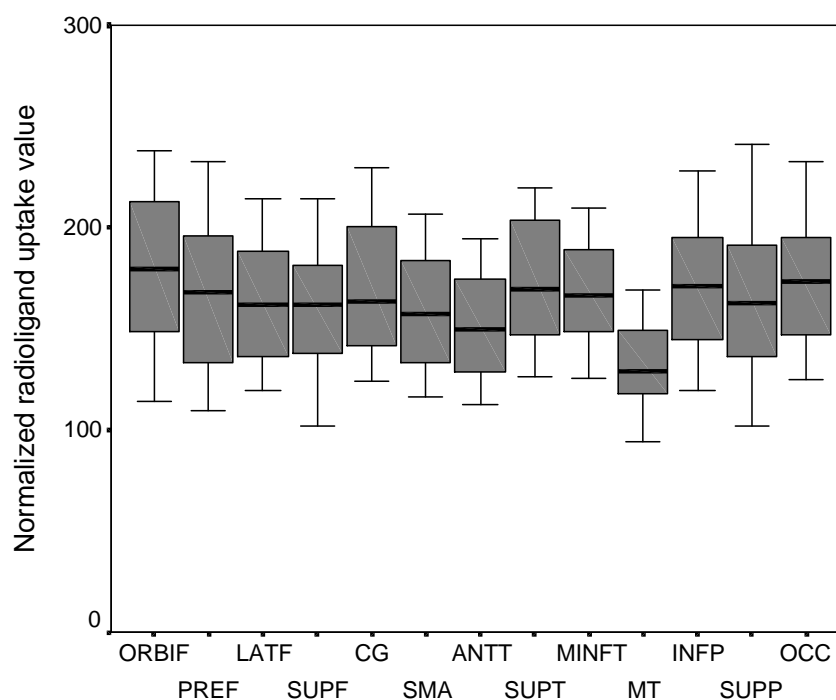


Figure 1. The distribution of radioligand uptake throughout the brain as measured in 26 healthy volunteers.

ORBIF = orbitofrontal; PREF = prefrontal; LATF = lateral frontal; SUPF = superior frontal; CG = cingulate gyri; SMA = sensorimotor area; ANTT = anterior temporal; SUPT = superior temporal; MINFT = medial inferior temporal; MT = mesotemporal; INFP = inferior parietal; SUPP = superior parietal; OCC = occipital

NEOCORTICAL BINDING POTENTIAL IN HEALTHY VOLUNTEERS AND RELATION WITH AGE AND GENDER

There was no statistically significant difference in radioligand uptake according to sex for any volume of interest. Concerning the age effect, the average neocortical binding potential varied between 217 at 23 years and 119 at 73 years. There was a significant age-related decline of neocortical binding potential (linear regression analysis: $R^2 = 0.87$, $p < 0.001$) resulting in an average decline of 11.6 ± 0.9 % per decade (figure 2). When only subjects over 60 years old were included, no significant age-related decline was present ($n = 13$; $R^2 = 0.1$, $p = 0.3$). Moreover, when only subjects over 70 years old were included ($n = 8$), the receptor binding potential as measured with ^{123}I -5-I-R91150 SPECT seemed to increase visually, however, this did not reach statistical significance ($p = 0.4$). The distribution of radioligand uptake throughout the brain compared between the 13 youngest (up to 52 years old) and the 13 oldest subjects (from 62 years on) is shown in figure 3. The highest age-related decline was reached in the posterior cingulate with a decrease of 14.2 % per decade ($R^2 = 0.78$, $p < 0.001$) while the lowest age-related decline was found in the left and the right mesotemporal region with a mean decrease of 7.6 % per decade ($R^2 = 0.8$, $p < 0.001$). There was no statistically significant asymmetry change according to age for any region.

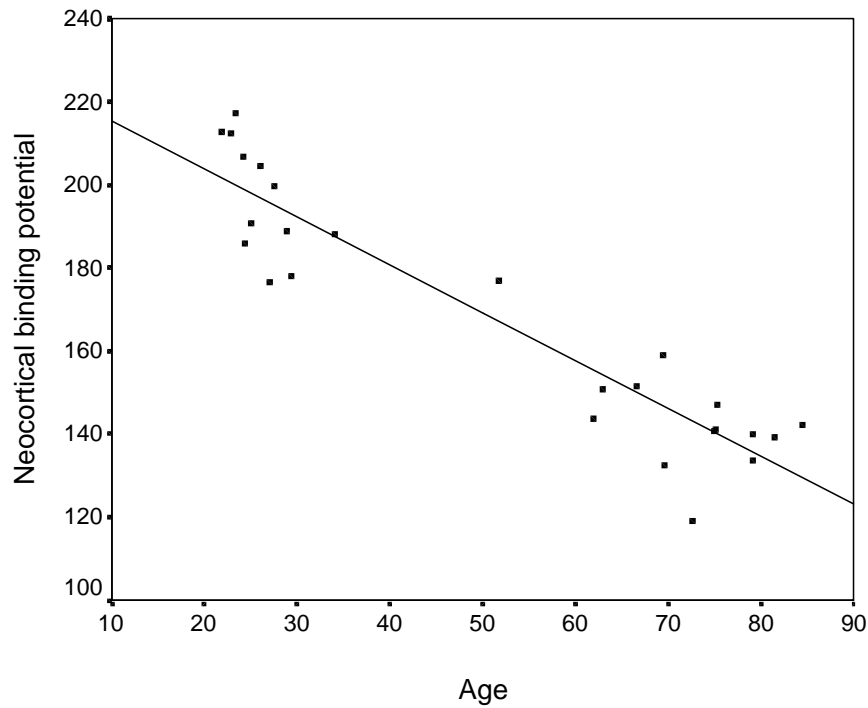


Figure 2. Age-related decline of the 5-HT_{2A} receptor neocortical binding potential as measured with ¹²³I-5-I-R91150 SPECT.

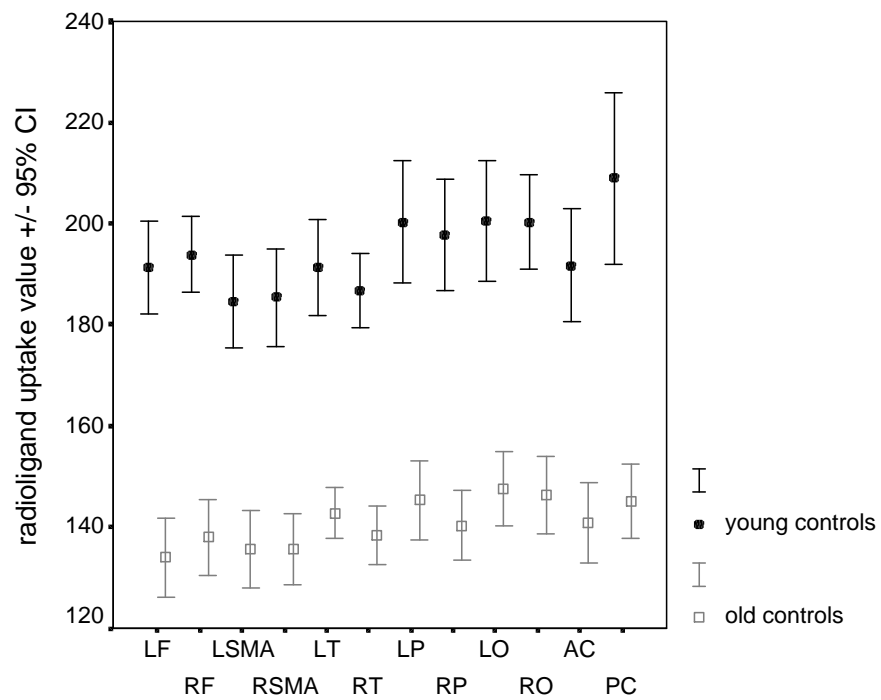


Figure 3. The distribution of radioligand uptake throughout the brain compared between the 13 youngest and the 13 oldest subjects (22-52 versus 62-85 yrs). LF = left frontal; RF = right frontal; LSMA = left sensorimotor; RSMA = right sensorimotor; LT = left temporal; RT = right temporal; LP = left parietal; RP = right parietal; LO = left occipital; RO = right occipital; AC = anterior cingulate; PC = posterior cingulate

ALZHEIMER'S DISEASE PATIENTS VERSUS AGE-MATCHED CONTROLS

Grouped mean uptake values for AD patients and age-matched controls are displayed in figure 4.

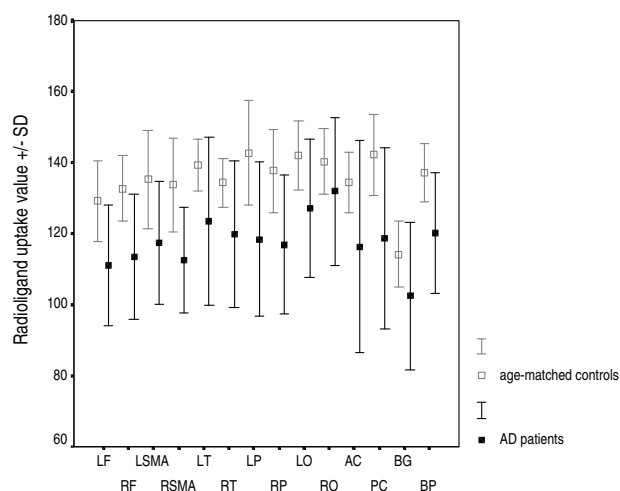


Figure 4. Grouped mean uptake values \pm SD for AD patients and age-matched controls.

A generally decreased neocortical binding potential was found in the AD patient group ($p = 0.02$). Mean regional uptake values for AD patients and controls are shown in Table 2.

	AD patients		age-matched controls		p-value, uncorrected
	UV	SD	UV	SD	
Orbitofrontal	117.6	21.5	139	14.5	0.04*
Prefrontal	107.7	18.6	126.7	12.3	0.03*
Lateral frontal	116.8	15.1	135.2	8.6	0.008*
Superior frontal	110.4	25.3	128.2	16.1	0.1
Cingulate gyri	117.3	25.4	137.7	7.6	0.02*
Sensorimotor	114.9	14.9	134.5	12.2	0.004*
Temporal anterior	112.3	24.8	128.7	10.9	0.2
Temporal superior	125.5	26.4	142.4	10.9	0.06
Temporal medial inferior	129.4	22.9	144.3	7.4	0.09
Mesotemporal	100.6	17.9	113.3	11.8	0.16
Parietal inferior	121.6	17.3	141.8	9.5	0.01*
Parietal superior	108.0	33.3	136.3	21.4	0.06
Occipital	129.5	19.3	141.2	8.2	0.04*

*statistically significant p-values

Table 2. ^{123}I -5-I-R91150 regional uptake values (UV) and standard deviation (SD) for AD patients compared to age-matched controls

For the individual regions, a statistically significant decreased binding potential in AD patients compared to controls was found in the orbitofrontal, prefrontal, lateral frontal, cingulate, sensorimotor, parietal inferior, and occipital region ($p_{\text{uncorrected}} < 0.05$). After Bonferroni correction for multiple comparisons, only the difference in radioligand uptake for the sensorimotor region yielded significance ($p = 0.05$).

Concerning asymmetries, a statistically significant asymmetry was found for the mesotemporal region in favor of the left side ($p = 0.02$). However, individually neither the left or right mesotemporal area differed significantly from age-matched controls concerning radioligand uptake.

Figure 5 shows the radioligand uptake values for AD patients and age-matched controls for the right sensorimotor and left orbitofrontal region. Figure 6 shows a representative slice of an age-matched healthy volunteer and an AD patient with the specific radioligand uptake decreases in the lateral frontal, sensorimotor, and posterior cingulate region.

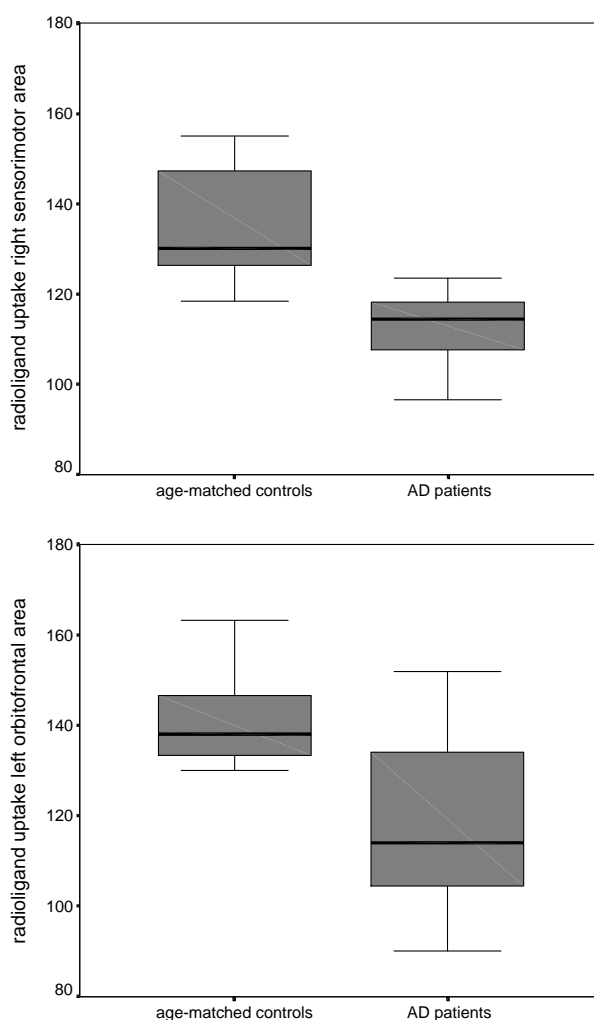


Figure 5. Boxplots of the ^{123}I -5-I-R91150 uptake values for AD patients and age-matched controls for the right sensorimotor (upper) and the left orbitofrontal (lower) region.

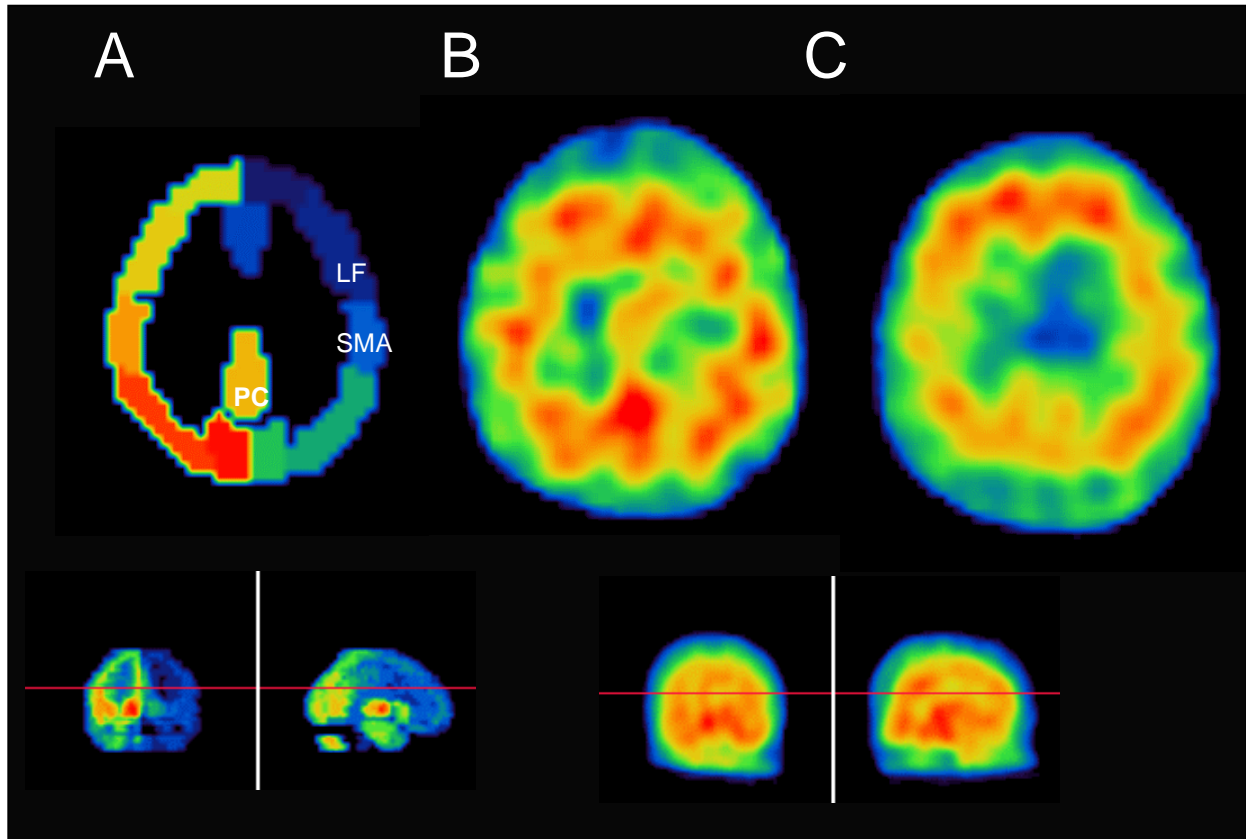


Figure 6. Figure of the VOI-map (A) together with a representative slice of an age-matched healthy volunteer (B) and an AD patient (C). Mark the cerebellum, representing free ligand and non-specific binding and also the specific uptake decreases in the lateral frontal (LF), sensorimotor (SMA) and the posterior cingulate region (PC) in the AD patient.

Neuropsychological testing and correlation with the ^{123}I -5-I-R91150 uptake values

The mean Mini-Mental State Examination score (MMSE) yielded 18 ± 6 (range 9-25). The mean score on the geriatric depression scale (GDS) was 9.1 ± 6 (range 2-19), where, according to the cut-offs used, two mildly and no severely depressed patients were included. No effect of depression score on regional or neocortical binding potential was present within the AD patient group. A significant positive correlation was found between the ^{123}I -5-I-R91150 uptake value in the left orbitofrontal region and the global cognitive deficit as assessed with the MMSE-score (Spearman's σ correlation coefficient of 0.7; $p < 0.05$). No correlation was found between ^{123}I -5-I-R91150 uptake values for any region and global or subscores on the ADS6 cognitive screening battery.

DISCUSSION

The present findings concerning age dependency of 5-HT_{2A} receptor density are in agreement with previous ex vivo distribution studies demonstrating a general decrease in cortical 5-HT and more specifically 5-HT_{2A} receptor density [39]. This decline is also consistent with clinical observations of age-related changes in behaviors such as sleep or executive functioning, known to be linked to serotonergic function [15,33]. Moreover, peak minus baseline prolactin responses to fenfluramine (a serotonin-releasing agent) were shown to be negatively correlated with age [26]. Concerning the regional age-dependent decreases in 5-HT_{2A} receptor density, a very recent study with [¹⁸F]altanserin found the highest age-related decline in the cingulate region while the lowest decline was found in the hippocampus, which is in concordance with the regional age-related decreases found in the present study [43].

This decrease in 5-HT_{2A} receptor density gradually declines, reaching a minimum between the 5th and the 6th decade [45]. As for in vivo imaging studies, several studies confirmed this linear decrease in cortical 5-HT_{2A} receptor binding in the living human brain with a more rapid decline in the first half of adult life, directly reflecting the loss of specific 5-HT_{2A} receptors with age [7,41,49]. Moreover, one study used the same radioligand as in the present study in a healthy control group up to 60 years old [4]. Also, it was previously shown that the effect of atrophy is relatively small compared to the large change in 5-HT_{2A} receptor binding in healthy aging [29]. The present study extends these previously published data since healthy subjects up to an age of 85 years were included where no significant age-related effect from the age of 60 on could be demonstrated. On the contrary, the receptor density seemed to slightly increase again from the age of 70, however, this did not reach statistical significance. This phenomenon of a parabolic relationship between aging and 5-HT_{2A} receptor density with an upswing from the age of 60 has also been reported previously for the prefrontal cortex and the hippocampal dentate using [³H]ketanserin autoradiography [22]. Concerning gender, our data could not show any significant gender difference in radioligand uptake for any brain region. Up till now only one PET study with [¹⁸F]altanserin, a 5-HT_{2A} receptor antagonist, has reported a gender difference in cortical 5-HT_{2A} receptor uptake in healthy subjects with a higher binding capacity in men in general with the greatest differences in the frontal and cingulate cortices [6].

Concerning the present findings about radioligand uptake in the AD patient group, our results are in line with previously published ex vivo data. Indeed, most postmortem studies showed, in addition to mostly frontal deficits, also deficits in cingulate and parietal 5-HT_{2A} binding sites [37]. However, an important issue concerning post-mortem studies is that some of these results, due to the nature of many of these studies, are potentially biased, firstly towards Alzheimer's disease of end-stage severity and secondly by post mortem delay. However, also two previously published PET studies with [¹⁸F]setoprone and [¹⁸F]altanserin showed this specific decrease in 5-HT_{2A} receptor density for AD patients, with the greatest deficits in frontal, cingulate, and temporal regions [7,28]. Interestingly, the reduction in radioligand uptake in the sensorimotor cortex, in fact the only statistically significant difference compared to age-matched

controls proof against formal Bonferroni correction, is somewhat unexpected but in line with recently published PET results using [^{18}F]altanserin [28]. Hypothetically, this could be related to a reduction in planned motor behavior and a reduction in sensory processing. Both aspects have been described in literature and are often observed in clinically demented patients [38,48].

Since binding potential may reflect changes in receptor density (B_{max}) as well as receptor affinity (K_D), abnormalities in either or both measures may contribute to the finding of a difference or, alternatively, a lack of difference in regional binding potential between different study groups. However, most postmortem binding assays and saturation binding experiments of 5-HT_{2A} receptor ligands in AD brains have shown abnormal B_{max} values and normal K_D values [12,13]. Therefore, it is likely that the low specific binding potential for several brain regions found in the present study is the result of a corresponding loss of 5-HT_{2A} receptors. This is similar to what has already been reported for most neuroreceptor changes in AD for e.g. the nicotinic, 5-HT₁, glutamate, NMDA, somatostatin or neuropeptide Y receptor sites [37].

Concerning the dynamic content of the measured receptor data, static scans were acquired and no full kinetic modelling of the receptor binding potential was measured. As mentioned already, pseudo-equilibrium conditions were assumed and the relative measure of neocortical to (nearly receptor-free) cerebellar activity was taken as a measure of the binding index, as has been shown in previous literature both by our group as well as others [3,4,11]. Under pseudo-equilibrium circumstances, the delivery phase of the tracer (initial flow) is not a determinant of the binding index anymore and therefore, regional estimates of perfusion need not to be correlated directly to the 5-HT_{2A} binding data.

No effect of depression score on global or regional binding potential was present within the AD patient group, although the low number of depressed subjects precluded a definitive examination of the 5-HT_{2A} receptor status in AD patients with concomittant depression. This is however in agreement with a previous PET study where no significant abnormalities in 5-HT_{2A} receptor binding potential as measured with [^{18}F]altanserin were observed in 11 patients with late-life depression according to DSM-IV and Hamilton depression scale criteria. Moreover, no effect of depression on neither global nor regional binding potential was present within the AD patient group (3 out of 11 with concurrent depression) [28]. These findings are consistent with the hypothesis that the 5-HT_{2A} receptor is differentially affected in late-life depression and AD, a finding that has implications for the etiological basis of mood and cognitive features of neuropsychiatric disorders of late life.

In conclusion, the results of the present study agree with and extend previous postmortem, in vitro and PET/SPECT in vivo findings. The age-related decline in 5-HT_{2A} receptor binding potential with a tendency towards a slight upswing towards later life highlights the necessity for age-matched controls in (clinical and) imaging studies and the need for larger study samples at advanced age. Moreover, it stresses the

etiological and potential therapeutic implications concerning mood changes and psychotropic drug dosing for older age groups. The fact that the 5-HT_{2A} receptor is differentially affected in AD patients compared to age-matched controls has implications for both the etiological basis and the therapeutic management of AD.

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SUMMARY, DISCUSSION AND PERSPECTIVES

The present thesis aims at being an aid in clarifying the pathophysiology of Alzheimer's disease by means of functional radionuclide imaging, this in order to reveal certain aspects of its disease process and finally aid its therapeutic management.

The option of functional radionuclide imaging being either positron emission tomography (PET) or single photon emission computed tomography (SPECT) was chosen because of its properties of allowing the non-invasive detection of specific cells and tissues involved in the pathophysiological process all depending of the radioligand of choice. This whereas the capability of structural imaging lies in visualising (mostly non-specific) structural changes and describing their detailed spatial relationship. As such, in general, the disease process must be already at an advanced stage before it can be depicted by structural imaging modalities, giving rise to its poor *pathophysiological sensitivity* at the early stages (when anatomical changes are not detectable yet). Also, for chronic processes like Alzheimer's disease, structural changes may be detectable that do not reflect the actual state of disease activity.

As for the newer structural or metabolic imaging tools however, for example *proton MR spectroscopy* seems more specific in assessing the pathophysiological process by means of for example measuring neurocellular viability or neuroaxonal integrity (N-acetyl aspartate) and glial (choline and especially myo-inositol) markers which, according to some authors, could be able to predict and monitor the response to therapy, giving rise to an individual optimised treatment. Likewise, *magnetisation transfer imaging* (MTI) seems valuable in measuring brain involvement and provides information about brain damage with increased pathological specificity detecting subtle microscopic abnormalities in brain tissue, which go undetected with conventional scanning. As such, a low MTI ratio indicates a reduced capacity of the macromolecules in brain tissue membranes to exchange magnetisation with the surrounding water molecules, reflecting damage to these membranes. Also, coefficients of water diffusion can be measured with *diffusion tensor MRI* where an increased water diffusivity reflects a disintegration of brain tissue compartments. As for *functional magnetic resonance imaging*, some studies suggest that fMRI can be used to diagnose Alzheimer's disease in its earliest stage, detecting subclinical deterioration of the memory function and may be useful to predict the future decline of memory in people with genetic or other risk factors.

This thesis is divided in two parts. One part (chapter two to six) deals with the *neuroinflammatory hypothesis* while the second part (chapter seven) deals with the *serotonergic hypothesis* in Alzheimer's disease.

In **chapter two**, in an *introductory section*, the epidemiology, clinical features, pathophysiology, and treatment of Alzheimer's disease is reviewed. A *second section* discusses three topics.

Firstly, the basic neuroinflammatory mechanisms and its biochemical characteristics, the potential

neurotoxic mediators during activation of microglia (i.e. the brain resident macrophages), and the current status of inflammation with respect to neurodegeneration is reviewed. Indeed, in the past decades, our understanding of the central nervous system has evolved from one of an immune-privileged site, to one where inflammation is pathognomonic for some of the most prevalent and tragic neurodegenerative diseases. Inflammation, whether in the brain or periphery, is almost always a secondary response to a primary pathogen. In head trauma, for example, the blow to the head is the primary event. What typically concerns the neurologist and neurosurgeon more, however, is the secondary inflammatory response that will ensue and likely cause more neuron loss than the initial injury. Current research indicates that diseases as diverse as multiple sclerosis, stroke and Alzheimer's disease exhibit inflammatory processes that contribute to cellular dysfunction or loss.

Secondly, the immune-related pathogenesis of Alzheimer's disease is thoroughly reviewed. It is clearly shown that inflammation contributes to neurodegeneration in Alzheimer's disease, not simply as a secondary phenomenon, but primarily as a significant source of pathology. As such, visualising this neuroinflammation would be of interest, firstly for clarifying the pathophysiology, secondly for selecting patient subgroups that are more eligible for anti-inflammatory treatment(s) and finally, for monitoring patients during trials with these anti-inflammatory agents.

Thirdly, the currently available neuroinflammatory imaging modalities, both structural and mainly functional, are critically reviewed and discussed. It is shown that, whereas structural imaging shows merely late anatomical consequences of an inflammatory response, functional imaging is a strong potential candidate to bridge the gap between *in vitro* and *in vivo* knowledge. In this perspective, a number of radioligands have been recently explored which allow the early *in vivo* visualisation of inflammatory responses, and, as such, open a promising window on both *understanding* as well as possible *clinical management* of inflammatory neurodegenerative disorders.

In the light of the aforementioned goals of neuroinflammatory imaging, a first attempt is made with ^{57}Co and SPECT. Indeed, previous studies showed that ^{57}Co SPECT is able to visualise inflammatory lesions, probably by means of the final common pathway of the Ca^{2+} -homeostasis disturbance in both neuronal degeneration and inflammation. **Chapter three** describes this attempt to visualise inflammation *in vivo* in Alzheimer's disease patients by detecting ^{57}Co SPECT changes and investigates whether ^{57}Co SPECT can generate additional information which cannot be obtained with conventional neuroimaging techniques or neuropsychological testing (NPT). As such, ^{57}Co SPECT data are compared with data obtained from Magnetic Resonance Imaging (MRI), perfusion SPECT, and neuropsychological testing, and finally findings in Alzheimer's disease patients are compared with patients suffering from vascular dementia and frontal lobe-type dementia. It is shown that ^{57}Co SPECT scans were not able to show any regional raised uptake and in this way ongoing tissue decay or inflammation, irrespective of the type of dementia, depth or extent of perfusion defects, presence of atrophy on MRI, or the results of NPT. In an attempt to explain these results it is concluded that the limitations of ^{57}Co SPECT are manifold. Due to the long physical half-life of 270 days, only a limited dose can be injected which is responsible for the low count rate and the resulting low statistics. Moreover, whether ^{57}Co visualises specific aspects of neuronal damage or blood-brain barrier integrity

is still uncertain. To what extent ^{57}Co really visualises calcium-mediated processes (*in vitro* and more importantly *in vivo*), and therefore resembles identical molecular uptake mechanisms, has yet to be determined, although the cerebral uptake of intravenously administered radioactive ^{45}Ca and ^{60}Co in neuronal damage is highly similar. Finally, its exact cellular site of accumulation of radioactivity is, as yet, not known.

After this, the development and validation of another radioligand for the visualisation of neuroinflammatory lesions is described. Indeed, the peripheral benzodiazepine receptor (PBR) was reported to reflect neuro-inflammatory damage by an upregulation on activated microglia. As such, radiolabelled PK11195, a high affinity ligand for the PBR, could be an ideal candidate. In **chapter four**, the biodistribution and dosimetry of [^{123}I]iodo-PK11195, a potential SPECT radioligand is described in humans. For this, sequential whole body scans were performed up to 72 hours post-injection of ^{123}I labelled iodo-PK11195. Multiple blood samples were taken, and urine was collected to measure the fraction voided by the renal system. Decay corrected regions of interest of the whole-body images were analysed, and geometric mean count rates were used to determine organ activity. Organ absorbed doses and effective dose were calculated using the MIRD method. It was seen that [^{123}I]iodo-PK11195 was rapidly cleared from the blood, mainly by the hepatobiliary system. Approximately 22% was voided in urine after 48 hours. Average organ residence times were 0.74, 0.44, and 0.29 hrs for the liver, upper large intestine, and lower large intestine respectively. The testes received the highest dose, 109.4 $\mu\text{Gy}/\text{MBq}$. All other organs investigated received doses of less than 50 $\mu\text{Gy}/\text{MBq}$. The effective dose was 40.3 $\mu\text{Sv}/\text{MBq}$. It was concluded that ^{123}I labelled iodo-PK11195 is a suitable agent for the visualisation of the PBR and indirectly for the imaging of neuroinflammatory lesions. Taking into account the radiation burden of 7.46 mSv following an administration of 185 MBq, a ^{123}I labelled iodo-PK11195 investigation should as such be considered as an ICRP risk category IIb investigation.

Thereafter, in **chapter five**, the validation of radiolabelled PK11195 as a neuroinflammatory tracer is described, this by applying the radiolabelled ligand in multiple sclerosis, the prototype neuroinflammatory disorder with its pathophysiological involvement of microglia. In an *introductory section*, the history, epidemiology, pathophysiology, clinical features and disease course, and treatment of multiple sclerosis is reviewed. In a *second section*, the visualisation of activated microglia in multiple sclerosis patients using [^{11}C]PK11195 and PET is studied. For this, semiquantitative [^{11}C]PK11195 uptake values were assessed for multiple sclerosis patients compared to healthy controls with a normalisation on cortical gray matter. It was found that the radioligand uptake in Gadolinium-lesions was significantly increased compared to normal white matter. Uptake in T2-lesions was generally decreased, suggesting a PBR downregulation. However, uptake values for T2-lesions increased whenever a clinical or MR-relapse was present, all suggestive for a dynamic process with a transient PBR upregulation. During disease progression, an increase of normal-appearing white matter (NAWM) radioligand uptake was found, propagating NAWM as the possible real burden of disease. It was concluded that [^{11}C]PK11195 PET imaging has an additional value over MRI concerning the immuno-pathophysiological process and is able

to demonstrate inflammatory processes with microglial involvement in multiple sclerosis. In a *third section* of this chapter, brain atrophy and microglial activation was assessed in multiple sclerosis patients during different disease stages and the relationship between inflammation, atrophy, and clinical measures was investigated. It was found that atrophy was significantly greater in multiple sclerosis patients compared to age-matched controls. Moreover, a significant correlation was found between brain atrophy and both disease duration and disability, as measured with the expanded disability status scale (EDSS). For NAWM, microglial activation as measured with [¹¹C]PK11195 uptake increased with the amount of atrophy, while T₂-lesional [¹¹C]PK11195 uptake values decreased according to increasing brain atrophy. It was concluded that brain atrophy, correlating with disease duration and disability, is directly related to NAWM and T₂-lesional inflammation as measured by this *PET probe* for microglial activation.

Chapter six describes the assessment of microglial activation using radiolabelled PK11195 for SPECT in Alzheimer's disease and its relation with findings obtained from perfusion SPECT and neuropsychological testing. For this, [¹²³I]iodo-PK11195 SPECT images were realigned into stereotactic space where binding indices, normalized on cerebellar uptake, were calculated. It was found that the mean [¹²³I]iodo-PK11195 uptake was increased in Alzheimer's disease compared to controls in nearly all neocortical regions, however, statistical significance was only reached in the frontal and right mesotemporal regions. Significant correlations were found between regional increased [¹²³I]iodo-PK11195 uptake values and specific cognitive deficits as assessed with neuropsychological testing. It is concluded that [¹²³I]iodo-PK11195 is a cellular disease activity marker allowing the *in vivo* assessment of microglial inflammation in Alzheimer's disease. Future optional work could be both at a technical and clinical level. Technically, a direct comparison between the PET and SPECT radioligand should be accomplished whereas feasible methods for absolute quantification of radioligand uptake should be further validated and implemented. From the clinical level, the inclusion of more patients at different stages of the disease, the comparison with proton MR spectroscopy for the measurement of glial markers, or the assessment of radioligand uptake changes during (anti-inflammatory) therapy could be very useful. Also, new ligands could be developed for the neuroinflammatory visualisation depending on the eventual development of the current anti-inflammatory treatment of choice. Ideally, this new radioligand should be rapidly cleared from blood and other non-target tissues and moreover, the interaction of the ligand and its receptor should be characterized by a high binding affinity and specificity (shown by autoradiography, receptor blockade, or studies with control agents). For neuroimaging studies in pathologies without blood-brain barrier breakdown (like Alzheimer's disease), the ligand should be able to easily penetrate this blood-brain barrier.

In a second part of this thesis (**chapter seven**) dealing with the serotonergic hypothesis of Alzheimer's disease, the role and distribution of serotonin (5-HT) type 2A receptors in healthy controls and Alzheimer's disease patients is described. In an *introductory section* the role of serotonin in general and serotonin type 2A receptors specifically in cognitive and non-cognitive behaviour and its relation with Alzheimer's disease in general and the inflammatory hypothesis more specifically is briefly

reviewed. In a *second section*, the imaging of the 5-HT_{2A} system in healthy controls and Alzheimer's disease patients is performed. Using ¹²³I-5-I-R91150, a selective radio-iodinated 5-HT_{2A} receptor antagonist and SPECT, the 5-HT_{2A} binding potential (BP) in healthy volunteers and Alzheimer's disease patients is calculated. For this, a semiquantitative analysis with normalisation on cerebellar uptake provided estimates of BP for 26 cortical regions of interest. An age-related decline of neocortical BP was found in healthy controls (11.6 % per decade). Compared to age-matched controls, a generally decreased neocortical BP in Alzheimer's disease was seen with a significant regional reduction in the orbitofrontal, prefrontal, lateral frontal, cingulate, sensorimotor, parietal inferior, and occipital region. These results are in line with previous postmortem, *in vitro*, and PET findings. As such, the age-related decline highlights the necessity for matched advanced age study samples. The fact that the 5-HT_{2A} receptor is differentially affected in Alzheimer's disease patients compared to controls has implications for both its etiological basis and therapeutic management.

As presented in the aforementioned manuscripts, both *neuroinflammatory* and *serotonergic* imaging yield different specific regional changes in binding potential for Alzheimer's disease patients, which raises the question of their (inter)relationship in terms of the Alzheimer's disease pathophysiology. Unfortunately, for reasons of logistics, no study was performed where both radiolabelled PK11195 and ¹²³I-5-I-R91150 was used in the same patients, however, one can assume that both populations included in these two studies are, however small, representative for a, if existing, *true* Alzheimer's disease population making these differences in regional binding potential changes in fact *true differences* reflecting as such not differences in the characteristics of the patients included, but reflecting a different point of view or part regarding the Alzheimer's disease pathophysiology. In fact, there are three options. Firstly, there is the notion of disease heterogeneity where questions have been raised about the existence of Alzheimer's disease as a single nosological entity. Although many researchers have tried to unify the different hypotheses concerning the aetiology and pathophysiology of Alzheimer's disease, many scientific arguments exist pointing to the possibility that there may not be just one *Alzheimer's disease* we are looking at. Indeed, many authors have raised the option of Alzheimer's disease patients with for example different neuropsychological or clinical profiles or different perfusion disturbances, not to mention the overlap both concerning risk factors and concerning clinical presentation between Alzheimer's disease and vascular dementia. Secondly, there is the option of a chronology in the pathophysiology of Alzheimer's disease in which different *brain systems* are more or less affected during the disease time course. In the light of the present thesis, the *series of events* presented here would be firstly the inflammatory response following a primary event (amyloid burden, ...) followed by functional neurotransmitter or more specifically serotonergic changes finally followed by structural changes like atrophy. Thirdly, there is the option of a co-existence of pathophysiological changes at the same time with a different regional sensitivity explaining these differences in regional binding potential changes. Indeed, one can speculate why the sensorimotor cortex is spared regarding perfusion but heavily affected concerning the 5-HT_{2A} system or why the mesotemporal area is largely affected by tissue loss and relatively spared concerning the serotonergic system.

To answer these and other questions it would be worthy to study in the same patients several pathophysiological points of view for example amyloidogenic, neuroinflammatory, perfusion, cholinergic, serotonergic and structural changes and this on different time points in order to label different pathophysiological mechanisms to different time courses of the disease. Ideally, this should also be done making use of different markers for measuring the same aspect of its pathophysiology, for example both neuroimaging (structural, functional, and metabolic), laboratory (serum, CSF, ...) as post-mortem neuropathological markers. This certainly, in an era where more and more treatment is available in order to be of any help in deciding when to apply which kind of treatment.

SAMENVATTING, DISCUSSIE EN TOEKOMSTPERSPECTIEVEN

Het huidige proefschrift tracht een hulp te zijn bij de opheldering van de pathofysiologie van de ziekte van Alzheimer door middel van functionele beeldvorming met behulp van radionucliden, dit om uiteindelijk aspecten van het ziekteproces te doorgronden and finaal mogelijks het therapeutisch beleid te beïnvloeden.

De optie van functionele beeldvorming zij het òfwel *positron emissie tomografie* (PET) ofwel *enkelvoudige foton emissie tomografie* (*single photon emission computed tomography* of SPECT) was verkozen gezien deze techniek ons in staat stelt tot een niet invasieve detectie van specifieke cellen en weefsels betrokken bij het pathofysiologisch proces, dit afhankelijk van het gekozen radioligand. Dit staat haaks tegenover de mogelijkheid van structurele beeldvorming die zich meer situeert in het in beeld brengen van (meestal aspecifieke) structurele veranderingen en het beschrijven van de gedetailleerde ruimtelijke relatie hiervan. Zodoende dient in het algemeen het ziekteproces reeds in een geavanceerd stadium te zijn vooraleer het kan gedetecteerd door middel van structurele beeldvormingsmodaliteiten wat aanleiding geeft tot zijn minder goede *pathofysiologische gevoeligheid* in de eerste stadia van de ziekte, wanneer anatomische veranderingen nog niet detecteerbaar zijn. Bovendien kunnen voor chronische aandoeningen zoals de ziekte van Alzheimer structurele veranderingen detecteerbaar zijn die de huidige ziekte-toestand niet correct weergeven.

Wat betreft de nieuwere structurele of metabole beeldvormingsmodaliteiten echter lijkt bijvoorbeeld *proton MR spectroscopie* meer specifiek in het in kaart brengen van het pathofysiologisch proces, dit door middel van het meten van neurocellulaire viabiliteits- of neuro-axonale integriteits- (N-acetyl-aspartaat) en gliale (choline en vooral myo-inositol) merkers die, volgens sommige auteurs, in staat zijn om het antwoord op de ingestelde therapie te voorspellen en te volgen mogelijks leidend tot een geïndividualiseerde meer optimale behandeling. Evenzeer lijkt *magnetisation transfer imaging* (MTI) waardevol in het meten van de betrokkenheid van het brein in het ziekteproces en verschaft zodoende informatie over hersenschade met een verhoogde pathologische specificiteit door subtiële microscopische abnormaliteiten in het hersenweefsel te ontdekken welke nog niet gedetecteerd kunnen worden met conventionele beeldvormingsmodaliteiten. In die zin zou een verlaagde MTI ratio op een verminderde capaciteit wijzen van de macromoleculen in de membranen van het hersenweefsel om magnetisatie uit te wisselen met de omgevende watermoleculen wijzend op schade aan deze membranen. Verder kunnen coëfficiënten van waterdiffusie gemeten worden met behulp van *diffusion tensor MRI* waarbij een verhoogde waterdiffusie-coëfficiënt een desintegratie van hersenweefselcompartimenten reflecteert. Wat betreft functionele magnetische resonantiebeeldvorming (fMRI) suggereren sommige studies dat fMRI in staat zou zijn om de ziekte van Alzheimer in een vroegtijdig stadium te diagnosticeren door het detecteren van subklinische deterioraties van de geheugenfunctie waardoor het in die zin nuttig zou kunnen zijn om toekomstig geheugenverlies te voorspellen en dit vooral bij mensen met genetische of andere risicofactoren.

Het huidige proefschrift is opgedeeld in twee delen. Eén deel (hoofdstuk twee tot en met zes) behandelt de *neuro-inflammatoire hypothese*, terwijl het tweede deel (hoofdstuk zeven) de *serotonerge hypothese* bij de ziekte van Alzheimer behandelt.

In **hoofdstuk twee** wordt in een *inleidende sectie* de epidemiologie, klinische verschijnselen, pathofysiologie en de behandeling van de ziekte van Alzheimer toegelicht. Een *tweede sectie* bediscussieert drie topics.

In een eerste topic wordt de basis omtrent neuro-inflammatoire mechanismen en zijn biochemische karakteristieken, de mogelijk neurotoxische mediators tijdens de activatie van microglia (de hersenmacrofagen) en de huidige status met betrekking tot inflammatie en neurodegeneratie toegelicht. Inderdaad, in de laatste decades is ons begrip van het centraal zenuwstelsel geëvolueerd van dat van een immuun-geprivilegeerde plaats tot dat van een plaats waar inflammatie kenmerkend is voor enkele van de meeste voorkomende en tragische neurodegeneratieve aandoeningen. Inflammatie, zij het centraal of perifeer, is meestal een secundaire respons op een primair pathogeen. Bij een hoofdtrauma bijvoorbeeld is de slag op het hoofd het primaire event. Wat de neuroloog en de neurochirurg vooral zal interesseren echter is de secundaire inflammatoire respons die erop zal volgen en mogelijks meer neuronale verlies zal berokkenen dan het initieel incident. Huidig onderzoek wijst erop dat ziektes zoals multiple sclerose, beroerte en de ziekte van Alzheimer inflammatoire processen vertonen welke een bijdrage leveren tot het verlies of de disfunctie van neuronale cellen.

Ten tweede wordt de immuungerelateerde pathogenese van de ziekte van Alzheimer grondig toegelicht. Het wordt duidelijk dat inflammatie bijdraagt tot neurodegeneratie in de ziekte van Alzheimer, dit niet enkel als een secundair fenomeen maar ook primair als een significante bron van pathologie. In die zin zou het in beeld brengen van deze inflammatie interessant zijn, ten eerste voor een bijdrage te leveren wat betreft de kennis van de pathofysiologie, ten tweede voor het selecteren van patiëntengroepen die in aanmerking zouden komen voor behandeling met (een) anti-inflammatoire therapie(ën) en ten slotte voor het opvolgen van deze patiënten tijdens deze trials met anti-inflammatoire medicatie.

Ten derde wordt de huidige stand van zaken omtrent neuro-inflammatoire beeldvormingsmodaliteiten en dit zowel structureel als vooral functioneel kritisch toegelicht en bediscussieerd. Het wordt duidelijk dat, terwijl structurele beeldvorming meestal late anatomische veranderingen van een inflammatoire respons aantoont, functionele beeldvorming een sterke kandidaat is om de kloof tussen *in vitro* en *in vivo* kennis te dichten. In dit perspectief zijn recent een aantal radioliganden bestudeerd die ons toelaten tot het vroeg *in vivo* visualiseren van inflammatoire veranderingen en op die manier een perspectief bieden op zowel *het begrijpen* als het uiteindelijke *klinische beleid* van inflammatoire neurodegeneratieve aandoeningen.

In het licht van deze hierboven vermelde objectieven van neuro-inflammatoire beeldvorming werd een eerste poging gedaan met ^{57}Co en SPECT. Inderdaad, vroegere studies wezen erop dat ^{57}Co SPECT in staat is om inflammatoire letsels in beeld te brengen dit mogelijks door middel van de *final common*

pathway van de Ca^{2+} -homeostase-stoornis en dit zowel in neuronale degeneratie als in inflammatie. **Hoofdstuk drie** beschrijft deze poging tot het in beeld brengen van inflammatie *in vivo* in patiënten met de ziekte van Alzheimer door middel van het detecteren van ^{57}Co SPECT veranderingen en investeert of ^{57}Co SPECT in staat is tot het genereren van additionele informatie die niet vergaard kan worden door middel van conventionele beeldvormingsmodaliteiten of neuropsychologische testen. In die zin werden ^{57}Co SPECT data vergeleken met data verkregen door middel van MRI, perfusie SPECT en neuropsychologische testen en werden deze resultaten bij patiënten lijdend aan de ziekte van Alzheimer vergeleken met deze van patiënten lijdend aan vasculaire en frontale dementie. Er wordt aangetoond dat ^{57}Co SPECT niet in staat is om regionaal verhoogde opnames en in die zin weefselverval of inflammatie in beeld te brengen en dit ongeacht van het type dementie, de ernst en de uitgebreidheid van de doorbloedingsdefecten, de aanwezigheid van atrofie op MRI noch van de resultaten van de neuropsychologische testen. In een poging om de hierboven vermelde resultaten te verklaren wordt geconcludeerd dat de beperkingen van ^{57}Co SPECT veelvuldig zijn. Door het lang fysisch halfleven van namelijk 270 dagen kan slechts een beperkte dosis geïnjecteerd worden hetgeen verantwoordelijk is voor de lage *count rate* en de resulterende lage beeldvormingsstatistieken. Bovendien is het nog steeds niet zeker of ^{57}Co specifieke aspecten van neuronale schade dan wel bloed-hersenbarrière-doorbraak in beeld brengt. In hoeverre ^{57}Co werkelijk Calcium-gemedieerde processen in beeld brengt (*in vitro* en nog belangrijker *in vivo*) en in die zin staat voor identieke moleculaire opnamemechanismen dient nog bepaald te worden, hoewel de cerebrale opname van intraveneus toegediend ^{45}Ca en ^{60}Co bij neuronale schade zeer veel gelijkaardige kenmerken vertoont. Tenslotte is de exacte cellulaire opnameplaats van de radioactiviteit nog niet gekend.

Hierna wordt de ontwikkeling en validatie van een nieuw radioligand voor de beeldvorming van neuro-inflammatoire letsels beschreven. Zo wordt gebruik gemaakt van de *perifere benzodiazepine receptor* (PBR) die in staat is om neuro-inflammatoire schade in beeld te brengen dit door middel van een upregulatie op geactiveerde microglia. Aldus zou radioactief gemerkt PK11195, een hoog-affiniteitsligand voor deze PBR, een ideale kandidaat zijn. In **hoofdstuk vier** wordt de biodistributie en dosimetrie van [^{123}I]iodo-PK11195, een potentieel SPECT radioligand beschreven bij mensen. Hiervoor worden sequentiële *whole body* opnames verricht tot 72 uur na de injectie van ^{123}I gemerkt iodo-PK11195. Meerdere bloedafnames werden verricht en de urine werd verzameld voor het meten van de fractie welke geklaard werd door het renaal systeem. Voor verval gecorrigeerde regio's van deze *whole body* opnames werden geanalyseerd en geometrisch gemiddelde activiteitsverdelingen werden gebruikt om orgaanactiviteiten te bepalen. De geabsorbeerde en de effectieve dosissen werden berekend gebruik makende van de MIRD methode. Er werd vastgesteld dat [^{123}I]iodo-PK11195 snel geklaard werd vanuit het bloed, dit hoofdzakelijk door het hepatobiliair systeem. Ongeveer 22% was terug te vinden in de urine na 48 uur. De gemiddelde orgaan-residentietijden waren 0.74, 0.44 en 0.29 uur voor de lever, bovenste dikke darm en onderste dikke darm respectievelijk. De testis ontvingen de hoogste dosis namelijk 109.4 $\mu\text{Gray}/\text{MBq}$. Alle andere organen ontvingen dosissen van minder dan 50 $\mu\text{Gray}/\text{MBq}$. De effectieve dosis was 40.3 $\mu\text{Sv}/\text{MBq}$.

Zodoende konden we concluderen dat [^{123}I]iodo-PK11195 een geschikt radioligand is voor de beeldvorming van de PBR en indirect voor de beeldvorming van neuro-inflammatoire letsels. Rekening houdend met de stralingsbelasting van 7.46 mSv na een toediening van 185 MBq kan men een [^{123}I]iodo-PK11195 onderzoek beschouwen als een ICRP risicocategorie IIB investigatie.

Hierna wordt in **hoofdstuk vijf** de validatie van radioactief gemerkt PK11195 als neuro-inflammatoir radioligand beschreven, dit door het toepassen ervan in multipale sclerose, het prototype van de neuro-inflammatoire aandoening met zijn pathofysiologische betrokkenheid van microglia. In een *inleidende sectie* wordt de historiek, epidemiologie, pathofysiologie, klinische kenmerken en ziekteverloop en de behandeling van multipale sclerose toegelicht. In een *tweede sectie* wordt de beeldvorming van geactiveerde microglia in multipale sclerose patiënten door middel van [^{11}C]PK11195 en PET bestudeerd. Hiervoor worden semi-kwantitatieve [^{11}C]PK11195 opnamewaarden berekend voor multipale sclerose patiënten en vergeleken met gezonde vrijwilligers, dit met een normalisatie ten opzichte van corticale grijze stof. Er wordt geconcludeerd dat de opname van het radioligand in gadoliniumletsels significant gestegen is in vergelijking met de opname in de normale witte stof. De opname in T₂-letsels is over het algemeen verminderd, suggestief voor een PBR downregulatie. Hiertegenover staat een toename van de opnamewaarden wanneer een klinische of MRI-opstoot aanwezig is, suggestief voor een dynamisch ziekteproces met een voorbijgaande PBR-upregulatie. Tijdens de ziekteprogressie wordt een toename van de opname van het radioligand bemerkt ter hoogte van de normaal-uitziende witte stof wat erop wijst dat deze normaal-uitziende witte stof aan de grondslag ligt van het ziekteproces. Als conclusie kunnen we stellen dat [^{11}C]PK11195 PET beeldvorming een additionele waarde heeft tegenover MRI wat betreft het immunopathofysiologisch proces, en in staat is om inflammatoire processen met een microgliale betrokkenheid aan te tonen in multipale sclerose. In een derde sectie van dit hoofdstuk werd hersenatrofie en microgliale activatie opgemeten in multipale sclerose patiënten tijdens de diverse ziektestadia en werd de relatie tussen inflammatie, atrofie en klinische evaluatieschalen geïntegreerd. Er werd vastgesteld dat atrofie significant toegenomen was bij multipale sclerose patiënten in vergelijking met leeftijdsgenoten. Bovendien was er een positieve correlatie tussen hersenatrofie en zowel ziekteduur als invaliditeit, dit laatste gemeten aan de hand van de *expanded disability status scale* (EDSS). Voor de normaal-uitziende witte stof was er een gestadige toename van microgliale activatie (gemeten met behulp van [^{11}C]PK11195 PET) en de hoeveelheid atrofie, dit terwijl de microgliale activatie ter hoogte van de T₂-letsels afnam naar gelang het toenemen van de hersenatrofie. Als besluit kunnen we stellen dat hersenatrofie correleert met ziekteduur en invaliditeit en gerelateerd is aan inflammatie ter hoogte van de normaal uitziende witte stof en de T₂-letsels dit gemeten door middel van deze *PET-probe* voor microgliale activatie.

Hoofdstuk zes beschrijft de meting van microgliale activatie door middel van radioactief gemerkt PK11195 voor SPECT bij de ziekte van Alzheimer en zijn relatie met de bevindingen verkregen door perfusie SPECT en neuropsychologische testen. Hiervoor werden [^{123}I]iodo-PK11195 SPECT beelden gerealigneerd in een stereotactische ruimte waarvoor bindingspotentialen (relatief ten

opzichte van het cerebellum) berekend werden. Er werd gemiddeld een verhoogde [¹²³I]iodo-PK11195 opname vastgesteld bij patiënten lijdend aan de ziekte van Alzheimer in vergelijking met controlepersonen en dit in bijna alle neocorticale regio's hoewel statistische significantie enkel bereikt werd in de frontale en rechter mesotemporale regio's. Directe correlaties werden gevonden tussen regionaal toegenomen [¹²³I]iodo-PK11195 opnamewaarden en cognitieve defecten. Zodoende kan men stellen dat [¹²³I]iodo-PK11195 een cellulaire marker is van de ziekteactiviteit die ons in staat stelt tot het *in vivo* evalueren van microgliale inflammatie bij de ziekte van Alzheimer. Toekomstig werk zou zowel technisch als klinisch kunnen zijn. Methodologisch zou er een directe vergelijking dienen te gebeuren tussen de PET en SPECT radioligand terwijl eveneens bruikbare methodes voor de absolute quantificatie verder gevalideerd en geïmplementeerd zouden moeten worden. Klinisch zou de inclusie van meer patiënten en dit tijdens verschillende ziektestadia, de vergelijking met proton MR spectroscopie voor de meting van gliale merkers of de evaluatie van wijzigingen in de opname van dit radioligand tijdens (anti-inflammatoire) behandelingsstrategieën zeer nuttig kunnen zijn. Evenzeer zouden nieuwe radioliganden ontwikkeld kunnen worden voor neuro-inflammatoire beeldvorming, afhankelijk van de eventuele ontwikkeling van nieuwere anti-inflammatoire behandelingsmodaliteiten. Idealiter moet dit nieuw radioligand in staat zijn om snel geklaard te worden uit het bloed en andere *non-target* weefsels en dient de interactie tussen het radioligand en de receptor gekenmerkt te zijn door een hoge bindingsaffiniteit en specificiteit, zoals aangetoond door middel van autoradiografie, receptorblokkadestudies of studies met controle-agentia. Voor neuro-beeldvormingsstudies bij pathologieën zonder bloed-hersenbarrière doorbraak (zoals bij de ziekte van Alzheimer) dient het radioligand tevens in staat te zijn deze snel en eenvoudig te kunnen penetreren.

In het tweede deel van dit proefschrift (**hoofdstuk zeven**) handelend over de serotonerge hypothese van de ziekte van Alzheimer wordt de rol en de verdeling van serotonine type 2A receptoren bij gezonde controlepersonen en patiënten lijdend aan de ziekte van Alzheimer beschreven. In een *inleidende sectie* wordt de rol van serotonine en vooral serotonine type 2A receptoren voor cognitief en niet-cognitief gedrag en zijn relatie met de ziekte van Alzheimer in het algemeen en de inflammatoire hypothese in het bijzonder kort geëxploreerd. In een *tweede sectie* wordt de beeldvorming van het 5-HT_{2A} systeem in gezonde vrijwilligers en patiënten lijdend aan de ziekte van Alzheimer beschreven. Gebruik makende van [¹²³I]-5-I-R91150, een selectief radioactief gemerkte 5-HT_{2A} receptor antagonist en SPECT wordt de 5-HT_{2A} bindingspotential in gezonde vrijwilligers en patiënten lijdend aan de ziekte van Alzheimer berekend. Hiervoor wordt een semi-kwantitatieve analyse (relatief ten opzichte van het cerebellum) verricht, welke bindingspotentialen oplevert voor 26 corticale regio's. Er werd een leeftijdsafhankelijke afname van de neocorticale bindingspotential gevonden voor gezonde vrijwilligers (11.6% per decade). In vergelijking met leeftijdsgenoten was er een algemeen gedaalde neocorticale bindingspotential in patiënten lijdend aan de ziekte van Alzheimer met een significant regionale vermindering in de orbitofrontale, prefrontale, lateraal frontale, sensorimotore, inferopariëtale en occipitale regio en de gyri cinguli. Deze resultaten zijn in overeenstemming met vroeger *post mortem*, *in vitro* en PET bevindingen. Aldus stelt deze leeftijdsafhankelijke afname de noodzaak in het licht voor *gematchte* hoogbejaarde studiegroepen.

Het feit dat de 5-HT_{2A} receptor aangetast is bij patiënten lijdend aan de ziekte van Alzheimer in vergelijking met leeftijdsgenoten heeft implicaties voor zowel de etiologie als het therapeutisch beleid hiervan.

Zoals vermeld bij de hierboven voorgestelde resultaten leveren neuro-inflammatoire en serotonerge beeldvorming verschillende specifieke regionale veranderingen in bindingspotentiaal op voor patiënten lijdend aan de ziekte van Alzheimer, hetgeen de vraag doet rijzen naar hun respectievelijke relatie met betrekking tot de pathofysiologie van de ziekte van Alzheimer. Jammer genoeg werd er om logistieke redenen geen enkele studie verricht waarbij zowel radioactief gemerkt PK11195 en ¹²³I-5-I-R91150 gebruikt werd bij dezelfde patiënten hoewel men kan veronderstellen dat beide populaties welke geïnccludeerd werden in deze twee studies, hoewel klein, toch representatief zijn voor een, indien ze al bestaat, *waarachtige* populatie van patiënten lijdend aan de ziekte van Alzheimer hetgeen de verschillen in regionale bindingspotentiaalwijzigingen tot *echte verschillen* maakt als dusdanig, niet wijzend op verschillen in de geïnccludeerde patiëntenkarakteristieken maar wijzend op een verschillend aspect van de pathofysiologie van de ziekte van Alzheimer. Hiervoor zijn er minstens drie mogelijke verklaringenmodellen. Ten eerste is er de notie van de heterogeniteit van de ziekte van Alzheimer waar vragen rijzen omtrent het bestaan van de ziekte van Alzheimer als een enkelvoudige pathofysiologische entiteit. Hoewel meerdere onderzoekers getracht hebben de verschillende hypothesen betreffende de etiologie en pathofysiologie van de ziekte van Alzheimer te verenigen, zijn er toch diverse wetenschappelijke argumenten wijzend op de mogelijkheid dat er niet één *ziekte van Alzheimer* bestaat. Inderdaad, reeds vele auteurs hebben gewezen op patiënten lijdend aan de ziekte van Alzheimer met bijvoorbeeld enerzijds verschillende neuropsychologische of klinische presentaties of anderzijds verschillende doorbloedingsstoornissen om nog maar te zwijgen over de overlap betreffende zowel risicofactoren als klinische presentatie tussen patiënten lijdend aan de ziekte van Alzheimer en patiënten lijdend aan vasculaire dementie. Ten tweede is er de optie van een chronologie in het pathofysiologisch proces van de ziekte van Alzheimer waarin verschillende hersensystemen min of meer aangetast zijn gedurende het ziekteproces. In het licht van de huidige thesis zou de hier voorgestelde opeenvolging van gebeurtenissen vooreerst de inflammatoire respons zijn, volgend op een primair event (amyloïde accumulatie, ...), hierna gevolgd door functionele neurotransmitter of meer specifiek serotonerge wijzigingen finaal gevolgd door structurele veranderingen zoals atrofie. Ten derde is er de optie van co-existentie van pathofysiologische veranderingen met een verschillende regionale gevoeligheid welke een verklaring bieden voor de verschillen in regionale bindingspotentiaalwijzigingen. Inderdaad kan men zich afvragen waarom de sensorimotore cortex relatief onaantast is wat betreft perfusie maar zwaar aangetast betreffende het serotonine 2A systeem of bijvoorbeeld de mesotemporale regio voornamelijk aangetast is door atrofie en relatief onaantast betreffende het serotonerge systeem.

Om deze en andere vragen te kunnen beantwoorden zou het waardevol zijn om verschillende pathofysiologische aangrijpingspunten bij dezelfde patiënten te bestuderen, bijvoorbeeld amyloïdogene, neuro-inflammatoire, cholinerge, serotonerge, perfusionele en structurele veranderingen en dit op verschillende tijdstippen van het ziekte-evolutie om zodoende in staat te zijn

de diverse pathofysiologische mechanismen te kunnen toeschrijven aan verschillende tijdstippen van het ziekteproces. Idealiter zou dit moeten gedaan worden gebruik makende van verschillende meetinstrumenten voor het evalueren van hetzelfde pathofysiologisch proces bijvoorbeeld zowel beeldvorming (structureel, functioneel en metabool), laboratoriuminvestigaties (bloed, cerebrospinaal vocht, ...) als post mortem neuropathologisch onderzoek. Dit zeker in een tijdstip waar meer en meer behandeling beschikbaar wordt om zodoende van enig nut te kunnen zijn bij de beslissing welke therapie wanneer toe te passen.

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CURRICULUM VITAE

Jan Jozef Albert Versijpt is geboren op 10 november 1972 te Sint-Amandsberg. Vanuit een basisinteresse voor wetenschappen met een humane *touch* koos hij in 1990 voor de artsstudie aan de Universiteit van Gent, welke hij in 1997 beëindigde. Steeds geboeid door de fysiopathologie van het menselijk brein leek het dan ook een ideale mogelijkheid om aansluitend te kunnen starten met wetenschappelijk onderzoek en dit handelend over de ziekte van Alzheimer en nucleaire functionele beeldvorming, onder het promotorschap van Prof. J. Korf (vakgroep Biologische Psychiatrie, Rijksuniversiteit Groningen) en het co-promotorschap van Prof. Dr. R.A. Dierckx (dienst Nucleaire Geneeskunde, Universitair Ziekenhuis Gent). Als dusdanig is Jan (co-)auteur van 27 manuscripten in geïndexeerde tijdschriften en van meer dan 50 communicaties op (inter)nationale congressen. Eveneens werd hij de laureaat van twee reisbeurzen uitgereikt door de *International Society of Cerebral Blood Flow and Metabolism* en won hij een prijs uitgereikt door het wetenschappelijk comité van het *Belgisch Genootschap voor Nucleaire Geneeskunde*. Blijvend geïnterigeerd door het *in vivo-tracer*-principe van nucleaire geneeskunde als specialiteit en gecharmeerd door de nauwe samenwerking van deze discipline met zowel basis – als toegepaste wetenschappen besloot hij in deze richting verder te gaan. Voor het verder afwerken van deze opleiding tot geneesheer specialist in de Nucleaire Geneeskunde was hij vanaf oktober 2001 tewerkgesteld op de dienst Inwendige Ziekten, AZ St. Jan te Brugge en is hij momenteel werkzaam in de Kliniek H. Familie te Gent, dienst Isotopen. Wat betreft vrije tijd houdt Jan zich vooral bezig met improvisatietheater, salsa en sport.

‘Wie herinnert zich niet in zijn kindsheid theoloog, in zijn jeugd metafysicus en op zijn mannelijke leeftijd fysicus geweest te zijn?’

Auguste Comte in *Cours de philosophie positive* (1842)

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