

1 *A comparison of strength and power characteristics prior to anterior cruciate ligament*  
2 *rupture and at the end of rehabilitation in professional soccer players*

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47 **ABSTRACT**

48 **Background:** Strength and power is often reduced on the involved vs. contralateral limb and  
49 healthy controls following anterior cruciate ligament (ACL) reconstruction but no study has  
50 compared to pre-injury values at the time of return to sport (RTS).

51 **Hypothesis:** Divergent recovery patterns in strength and power characteristics will be present  
52 at RTS relative to pre-injury baseline data and healthy matched controls.

53 **Study design:** Cohort study

54 **Level of evidence:** Level 3

55 **Methods:** Isokinetic strength tests, bilateral and single leg countermovement jumps (CMJ;  
56 SLCMJ) were measured prior to ACL rupture in 20 professional soccer players. These then  
57 had surgical reconstruction (ACL group) and completed follow up testing prior to RTS.  
58 Healthy controls (uninjured group) were tested at the same time as the ACL group pre-injury.

59 Values recorded at RTS of the ACL group were compared to pre-injury. We also compared the  
60 uninjured and ACL groups at baseline and RTS.

61 **Results:** Compared to pre-injury, ACL normalised quadriceps peak torque of the involved limb  
62 (% difference = -7%), SLCMJ height (% difference = -12.08%) and Reactive Strength Index  
63 modified (RSImod) (% difference = -5.04%) were reduced following ACL reconstruction. No  
64 significant reductions in CMJ height, RSImod and relative peak power were indicated at RTS  
65 in the ACL group when compared to pre-injury values but deficits were present relative to  
66 controls. The uninjured limb significantly improved quadriceps (% difference = 9.34%) and  
67 hamstring strength (% difference = 7.36%) from pre-injury to RTS. No significant differences  
68 from baseline were shown in SLCMJ height, power and reactive strength of the uninjured  
69 limb following ACL reconstruction.

70 **Conclusion:** Strength and power in professional soccer players at RTS following ACL  
71 reconstruction were often reduced compared to preinjury values and matched healthy controls.

72 **Clinical relevance:** Deficits were more apparent in the SLCMJ suggesting dynamic and  
73 multijoint unilateral force production is an important component of rehabilitation. Use of the  
74 uninjured limb and normative data to determine recovery may not always be appropriate.

## 75 **KEYWORDS**

76 Anterior cruciate ligament, strength, power, reactive strength, soccer

77

## 78 **INTRODUCTION**

79 Anterior cruciate ligament (ACL) injuries in elite soccer players incur a high burden <sup>2</sup>, with  
80 substantial time-loss and economic cost <sup>10</sup>. This traumatic event often results in surgical  
81 reconstruction and return to sport (RTS) time is on average ~ 8 months <sup>37</sup>. Although most elite  
82 athletes (83%) return to their pre-injury level of competition following ACL reconstruction <sup>22</sup>,  
83 this is often accompanied by an increased risk of ipsilateral <sup>17</sup> and contralateral <sup>18</sup> injury, early  
84 onset of posttraumatic osteoarthritis, and sports performance deterioration <sup>8,22-24</sup>.

85 Strength and power are reduced following ACL reconstruction <sup>29</sup>. Strength assessment has  
86 commonly included isokinetic testing of knee extension and flexion peak torque, with  
87 established excellent reliability scores documented <sup>1,14,38</sup>. Deficits in peak knee extension and

88 flexion torque are commonly displayed in the ACL reconstructed limb compared to the  
89 uninvolved side and healthy controls after rehabilitation at the time of RTS <sup>15,29</sup>. In addition,  
90 jump performance is often used to quantify dynamic multijoint force production and can  
91 discriminate rehabilitation status <sup>31,32</sup>. Countermovement jump (CMJ) performance variables  
92 can help practitioners to quantify neuromuscular qualities that underpin movements inherent  
93 to soccer such as sprinting, jumping, and change of direction <sup>13</sup>. However, it has been suggested  
94 that single leg dynamic tasks are more representative of limb strength due to their higher  
95 relative force demands<sup>7</sup>, whereas bilateral jumping and landing tasks occur at a higher velocity.  
96 Furthermore, compensation strategies are restricted to interjoint in unilateral movements,  
97 whereas bilateral jumping can provide more options to unload the ACL reconstructed limb via  
98 both interjoint and interlimb <sup>28</sup>. The differing demands of the bilateral and unilateral tasks may  
99 reveal specific deficits, warranting the inclusion of both in the assessment of neuromuscular  
100 performance for athletes during rehabilitation aiming to return to a high level of competition.

101 Research <sup>16-20,31,32,34,35</sup> assessing strength and power characteristics in athletes following ACL  
102 reconstruction has been limited mostly to cross-sectional studies at single time points or around  
103 the time of RTS. Residual deficits in vertical jump height, lower limb power, and reactive  
104 strength appear to be present following ACL reconstruction <sup>27,32,34</sup>. Lower quadriceps strength  
105 and reduced plyometric ability have also displayed associations with increased risk of  
106 contralateral reinjury <sup>17,18</sup>. However, the available research has used the contralateral limb or  
107 values from matched controls to determine if deficits are present. There is potential for  
108 deterioration of the uninvolved contralateral limb following surgery due to deconditioning/lack  
109 of exposure <sup>44</sup>. Without pre-injury baseline physical characteristics, it is impossible to  
110 determine if athletes have returned to previous strength and jump performance values. It is also  
111 unknown if matched controls provide an accurate representation of baseline / pre-injury  
112 performance. A prospective study monitoring strength and power qualities from tests that are  
113 commonly used as part of RTS assessment in elite soccer players before and after ACL rupture  
114 and reconstruction may help guide performance recovery and determine the accuracy of proxy  
115 measures, including the uninvolved limb and comparison values of healthy controls.

116 Our aim was to examine changes in strength and power performance following the completion  
117 of rehabilitation at the time of RTS compared to pre-injury baseline data and compared to  
118 healthy matched controls. Using these data, we examined how pre-injury benchmark data can  
119 be used to guide performance recovery and inform physical readiness as part of RTS decision  
120 making. Our specific research questions included: 1) to what extent performance metrics are

121 recovered at the time of RTS following ACL reconstruction; and 2) how accurate is the use of;  
122 a) the contralateral limb; and b) group / control normative data as proxy measures for  
123 determining performance recovery when pre-injury data exist.

## 124 **METHODS**

### 125 **Participants**

126 Twenty soccer players ( $24.7 \pm 3.4$  years; height =  $175.3 \pm 7.0$  cm; weight =  $69.5 \pm 10.7$  kg)  
127 participating in the Qatar Stars and Gas Leagues attended a periodic health evaluation between  
128 2017 and 2019, and subsequently went on to sustain an ACL rupture before undergoing ACL  
129 reconstruction (ACL group). The majority of ACL grafts were bone-patella-tendon bone  
130 (80%), with the remaining players (20%) all semitendinosus and gracilis hamstring tendon  
131 grafts. Only participants with no history of previous ACL injury / surgery, or other knee  
132 ligament or cartilage injury / surgery of either the operated or non-operated leg at the time of  
133 the periodic health evaluation were included. All athletes were treated at the same Orthopaedic  
134 and Sports Medicine Hospital. Rehabilitation was delivered 5 days per week and divided into  
135 early, intermediate, and advanced phases. The focus of the early phase was on controlling  
136 swelling, restoring range of motion and activation of the knee extensor and flexor muscles. The  
137 goal of the intermediate and advanced phases were to optimise muscle strength, proprioception,  
138 and neuromuscular control, and complete a phased running progression program. On  
139 completion of these phases, players took part in an on-field sports specific training and  
140 conditioning block.

141 We also recruited thirty-five (uninjured) controls ( $23.8 \pm 2.8$  years; height =  $173.8 \pm 5.4$  cm;  
142 weight =  $71.6 \pm 6.3$  kg) from the same leagues who attended pre-season screening at the  
143 national sports medicine institution and were randomly selected from a pool of 300 athletes.  
144 Inclusion was based on having no history of ACL injury and being free from any severe injury  
145 (defined as  $> 28$  days' time-loss) in the previous 12 months, verified via a national injury audit.  
146 Clubs competing in the stated leagues within Qatar regularly complete formalised strength and  
147 conditioning including resistance training, speed, agility and plyometrics. Before participating,  
148 all participants provided informed written consent and ethical approval was provided (IRB:  
149 F2017000227).

### 150 **Experimental approach to the problem**

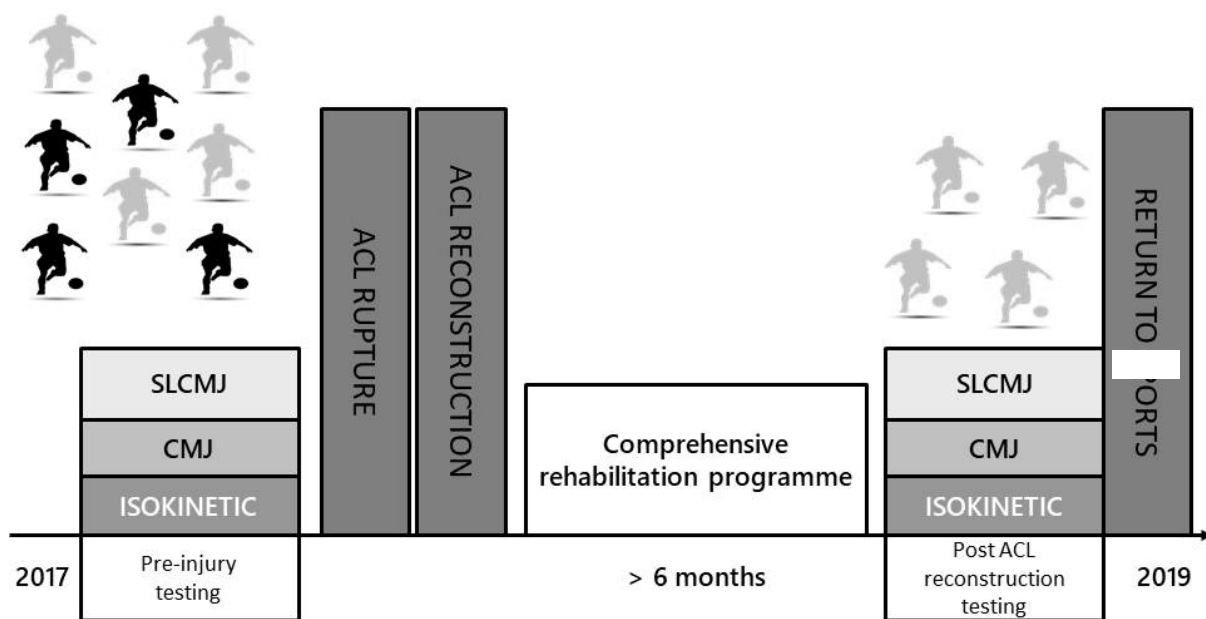
151 To address our stated aims, we separated the study into 4 components. *In part 1*, we compared  
152 strength and power characteristics of the ACL group to the uninjured group using both the pre-  
153 injury (baseline) data and performance following the completion of rehabilitation of the ACL  
154 group. Pre-injury baseline data are not commonly available, forcing clinicians to instead use  
155 either peers/published data and or the contralateral limb as proxy benchmarks following ACL  
156 reconstruction <sup>29</sup>, but the former has not been explored. In *part 2*, we monitored the trajectory  
157 of strength and power performance of the uninvolved limb in the ACL group by comparing  
158 isokinetic and SLCMJ assessment scores at two time points: pre-injury and at the end of  
159 rehabilitation prior to RTS. Conflicting evidence is available about the detrimental effect of  
160 ACL reconstruction and subsequent deconditioning on the uninvolved limb <sup>26,36,44</sup>. Currently,  
161 no study has conducted an assessment of strength and power characteristics of the uninvolved  
162 limb before and after ACL reconstruction following structured full time rehabilitation. In *part*  
163 *3*, we measured the effect of ACL reconstruction and rehabilitation on the injured limb by  
164 comparing isokinetic and SLCMJ performance scores at two time points: pre-injury and at the  
165 end of rehabilitation, following sports specific reconditioning prior to RTS. Finally, in *part 4*,  
166 we investigated the effect of ACL reconstruction on bilateral CMJ performance by comparing  
167 pre-injury and RTS values.

168

169

170 **Procedures**

171 A schematic diagram of our study is represented in Figure 1. A test battery consisting of  
 172 isokinetic strength assessment, CMJ, and SLCMJ was performed. The ACL reconstructed  
 173 cohort was screened  $33.9 \pm 29.6$  weeks before the ACL rupture, and assessed at the end of  
 174 rehabilitation prior to RTS ( $30.3 \pm 7.2$  weeks post-surgery). Players completed a standardized  
 175 warm up consisting of 5 minutes on a cycle ergometer, bilateral and unilateral bodyweight  
 176 squats, and bilateral CMJs at 50, 75 and 100% maximum effort <sup>33</sup>. Test conditions and  
 177 procedures were replicated at each assessment.



178  
 179 **Figure 1** Schematic representation of the study design. Uninjured players (black). Injured  
 180 players (grey).

181  
 182 *Isokinetic knee extension and flexion strength*

183 Maximal quadriceps knee extension peak torque (Quad PT Rel) and hamstring flexion peak  
 184 torque (HS PT Rel) relative to body mass ( $N \cdot m \cdot kg^{-1}$ ) were measured using an isokinetic  
 185 dynamometer (Biodex Medical Systems, Shirley, New York, USA). Players were in a seated  
 186 position with the hip flexed to  $90^\circ$ . Five repetitions of concentric knee extension and flexion  
 187 were performed at  $60^\circ/s$  with the highest peak torque value recorded <sup>42</sup>. Peak torque values  
 188 were reported as a percentage of the individual's body mass. Procedures were explained to  
 189 participants following which they completed 3 practice repetitions. Testing then commenced

190 after 60s. Limb order was randomized. The dominant limb of healthy controls was defined as  
191 the preferred kicking leg. Standardized, vigorous verbal encouragement was provided  
192 throughout. Each participant had previous experience of isokinetic testing and all tests were  
193 conducted by the same physiotherapist with > 5 years experience in the relevant test  
194 procedures.

195 *Countermovement Jump (bilateral/single)*

196 Participants were instructed to stand fully upright, hands on hips, and align their feet on a  
197 synchronized dual force plate system (ForceDecks v1.2.6109, Vald Performance, Albion,  
198 Australia). Prior to the initiation of the test, each individual was instructed to remain motionless  
199 for a minimum of three seconds to ensure a stable baseline of force at body weight was  
200 obtained. Players then performed a downward motion (descent phase) until they reached their  
201 preferred self-selected depth, before rapidly reversing the motion by triple extending at the hip,  
202 knee, and ankle. The aim of the task was to achieve their maximal



203 vertical displacement of the centre of mass. Hands remained on hips throughout and no bending  
204 of the knees was permitted whilst airborne. The procedures were replicated for the the SLCMJ,  
205 except the non-test leg was positioned with the hip and knee at 90° and no obvious swinging  
206 was allowed to minimize contralateral propulsion. Limb order was randomized. Two trials  
207 were performed with a 30 s rest period between each jump, with the best trial recorded for  
208 statistical analysis.

209 All data were recorded at a sampling rate of 1000 Hz. The initiation of the jump was defined  
210 by a 20 N change from body weight calculated during the quiet standing period and the instant  
211 of take-off, when the total vertical force dropped below 20 N. We selected three outputs, which  
212 are commonly reported in jump performing testing of healthy athletes and which can also be  
213 estimated using other lower cost technologies than force platform. Jump height was calculated  
214 from the impulse-momentum relationship derived take off velocity and equation of constant  
215 acceleration (velocity at take-off squared divided by  $2*9.81$  ( $v^2/2g$ ). Peak power was measured  
216 and normalized to bodyweight  $\text{Watt}\cdot\text{kg}^{-1}$  (Peak Power Rel) during the propulsion phase.  
217 Reactive strength index modified (RSImod) was calculated by dividing jump height by  
218 contraction time (determined from movement onset to time to take off<sup>39</sup>).

219 Intraday reliability analysis was conducted on baseline pre-injury scores of the ACL group.  
220 The between trial reliability was analyzed using a 2-way random effects intraclass correlation  
221 coefficient [ICC(2,1)]<sup>21</sup> with 95% confidence intervals (CI). The ICCs were analyzed as single  
222 measures. Coefficient of variation (CV%) and 95% confidence intervals (95%CI) and Standard  
223 error of measurement (SEM) were also calculated. Reliability scores were categorized as  
224 acceptable if the CV was  $\leq 10\%$ <sup>40</sup>, and were further categorized as “excellent” if ICC was  $>$   
225 0.90, “good” between 0.75 and 0.90, “moderate” between 0.50 and 0.75, and “poor”  $< 0.50$ <sup>21</sup>.

226 CMJ height, relative peak power and reactive strength displayed “excellent” reliability with  
227 ICC ranging from 0.945 to 0.978, and CV between 2.1 and 8.6% (Table 1). SLCMJ height,  
228 RSImod and jump height symmetry displayed “excellent” reliability, with ICCs ranging from  
229 0.901 to 0.960 and CV between 4.2 and 5.9 (Table 1). Relative peak power showed CV  $< 10\%$ ,  
230 and ICC between 0.781 and 0.860.

231

232

233 **Table 1** Intra-class correlation coefficients (ICC), coefficient of variation (CV%) and standard  
234 error of measurement (SEM) of the performance variables assessed during the bilateral  
235 countermovement jump (CMJ) and single leg countermovement jump (SLCMJ)

Test	Variable	CV % (95%CI)	ICC (2,1) (95% CI)	SEM
CMJ	Jump Height	2.7 (1.6 -3.8)	0.978 (.922- .994)	1.4
CMJ	Peak Power Rel	2.1 (1.2 – 3.0)	0.966 (.883- .991)	1.4
CMJ	RSI Mod	8.6 (5.0 – 12.2)	0.945 (.875-.976)	0.0
SLCMJ	Jump Height INV	5.2 (3.2 – 7.1)	0.96 (.876- .988)	1.0
SLCMJ	Peak Power Rel INV	6.3 (3.9 – 8.7)	0.781 (.424- .928)	2.2
SLCMJ	RSI Mod INV	10.8 (6.6 – 14.9)	0.907 (.724- .971)	0.0
SLCMJ	Jump Height UNINV	5.9 (3.6 – 8.1)	0.933 (.802-.979)	1.0
SLCMJ	Peak Power Rel UNINV	4.0 (2.5 – 5.5)	0.860 (.612- .955)	1.4
SLCMJ	RSI Mod UNINV	8.0 (4.9 – 11.1)	0.893 (.686- .966)	0.0
SLCMJ	Jump height symmetry	4.2 (2.4 - 6.0)	0.901 (.713- .968)	4.6

236 INV (involved limb), UNINV (uninvolved limb)

237

238

### 239 **Statistical analysis**

240 The distribution of the data were checked using the Shapiro-Wilk normality test. Descriptive  
241 statistics (mean  $\pm$  SD) for all variables were calculated. Percentage changes from pre-injury  
242 to post ACL reconstruction were calculated for each player using the percentage difference and  
243 then averaged.

244 In *part 1*, an independent samples *t*-test or Mann–Whitney U tests were used to examine  
245 differences in anthropometrics and physical performance variables between ACL and  
246 uninjured group.

247 For *parts 2, 3, and 4* paired-samples tests or Wilcoxon Rank Sum Test were used to detect  
248 statistical differences between pre-injury and post-surgery physical performance variables. The  
249 Two-way repeated measures ANOVA was used to examine the influence and interaction of  
250 time and/or injury (performance on the injured limb) for each test variable in the ACL group.

251 In all parts, Bonferroni correction was applied to reduce the risk of type I error with multiple  
252 statistical tests (adjusted  $\alpha = 0.025$  and  $\alpha = 0.017$  for isokinetic dynamometry and dual force

253 plate system derived variables respectively). Hedges *g* effect sizes (ES) with 95% confidence  
 254 intervals were calculated to interpret the magnitude of these differences with the following  
 255 classifications: standardized mean differences of 0.2, 0.5, and 0.8 for small, moderate, and  
 256 large effect sizes, respectively <sup>41</sup>. Significance was set at  $p < 0.05$ . Data processing and  
 257 descriptive statistics were processed using SPSS® (V.25. Chicago Illinois).

## 258 RESULTS

### 259 Part 1: strength and power characteristics of the ACL reconstructed group vs healthy 260 matched controls

261 Baseline (pre-injury) anthropometric, strength and power characteristics of the ACL  
 262 reconstructed group were not significantly different to healthy matched controls (see Table 2).

263 **Table 2** Isokinetic, single leg and bilateral countermovement jump (CMJ) results of each group

Test	Group 1 Pre-Injury (n=20)		Group 2: Healthy Controls (n=35)	Pre- injury vs controls effect size (95%CI)	Pre- injury vs controls <i>P</i> value
	Involved limb	Uninvolved limb	Dominant Limb		
<b>Quad PT Rel (N.m.kg<sup>-1</sup>)</b>	3.2±0.37	3.13±0.44	3.06±0.4	0.35 (- 0.21 to 0.92)	0.200
<b>HS PT Rel (N.m.kg<sup>-1</sup>)</b>	1.75±0.26	1.79±0.3	1.68±0.22	0.29 (- 0.27 to 0.86)	0.335
<b>SLCMJ Jump Height (cm)</b>	18.5±4.4	19.2.2±3.4	18.8±2.3	-0.09 (- 0.65 to 0.47)	0.787
<b>SLCMJ RSI Mod</b>	0.22±0.08	0.24±0.07	0.24±0.05	-0.25 (- 0.82 to 0.31)	0.510
<b>SLCMJ Peak Power Rel (W/Kg)</b>	31.7±4.3	32.7±4.4	31.9±4.2	-0.05 (- 0.61 to 0.52)	0.855
<b>CMJ Jump Height (cm)</b>	36.4±7.4		37.5±3.6	-0.22 (- 0.78 to 0.35)	0.231
<b>CMJ RSI Mod</b>	0.46±0.11		0.49±0.07	-0.30 (- 0.86 to 0.27)	0.354
<b>CMJ Peak Power Rel (W/Kg)</b>	52.1±6.3		52.8±4.9	-0.13 (- 0.69 to 0.44)	0.695

264 PT (peak torque), Rel (relative to body mass), N (Newtons), m (meters), kg (kilograms), W  
 265 (Watts), cm (centimeters)

266 Normalised quadriceps and hamstring peak torque were significantly higher in the uninvolved  
 267 limb of the ACL group prior to RTS compared to those who were uninjured ( $g = 0.77$ , 95%CI  
 268 [0.19, 1.36];  $p = 0.018$ , and  $g = 0.77$ , 95%CI [0.19, 1.35];  $p = 0.005$  respectively). There were  
 269 no significant differences in SLCMJ height, RSImod and relative peak power between the  
 270 uninvolved limb of the ACL group and uninjured controls (Table 3).

271 Normalised hamstring peak torque was significantly higher in the reconstructed limb of the  
 272 ACL group following rehabilitation compared to uninjured controls ( $g = 1.32$ , 95%CI [0.70,  
 273 1.93];  $p \leq 0.0001$ ), whereas there were no significant between-group differences in normalised  
 274 quadriceps peak torque (Table 4).

275 There were large significant differences between the ACL group following surgery and  
 276 uninjured controls in SLCMJ height ( $g = -1.64$ , 95%CI [-2.28, -0.99];  $p \leq 0.0001$ ), RSImod ( $g$   
 277  $= -0.93$ , 95%CI [-1.52, -0.34];  $p = 0.004$ ), and jump height symmetry ( $g = -1.51$ , 95%CI [-2.14,  
 278 -0.87];  $p \leq 0.001$ ) (Table 4).

279 There were large significant differences between the ACL group following surgery and  
 280 uninjured controls in CMJ height ( $g = -1.17$ , 95%CI [-1.77, -0.56];  $p \leq 0.0001$ ) and RSImod ( $g$   
 281  $= -0.89$ , 95%CI [-1.48, -0.30];  $p = 0.001$ ). Moderate differences in relative peak power ( $g = -$   
 282  $0.76$ , 95%CI [-1.34, -0.18];  $p = 0.008$ ) were also present between groups (Table 5).

283

284 **Table 3** Isokinetic and single leg countermovement jump (SLCMJ) results of the uninvolved  
 285 limb of the injured group and healthy matched controls

Test	Group 1 Pre- Injury (n=20)	Group 1 Post- Injury (n=20)	PRE vs POST effect size (95%CI)	PRE vs POST P value	Pre-Post Percentage difference (95%CI)	Group 2: Health y vs inju ry vs contr ols effect size (95% CI)	Post- injur y vs contr ols effect size (95% CI)	Post - inju ry vs cont rols P valu e
	Uninvolv ed limb	Uninvolv ed limb				Controls (n=35)		
<b>Quad PT Rel (N.m.k g<sup>-1</sup>)</b>	3.13±0.4 4	3.39±0.45	-0.57 (-1.23 to 0.08)	0.021	9.34% (6.45 to 12.23)	3.06±0. 4	0.77 (0.19 to 1.36)	<b>0.01 8</b>

<b>HS PT Rel (N.m.kg<sup>-1</sup>)</b>	1.79±0.3	1.87±0.29	-0.27 (-0.91 to 0.38)	0.261	7.36% (5.08 to 9.64)	1.68±0.22	0.77 (0.19 to 1.35)	<b>0.005</b>
<b>SLCMJ Jump Height (cm)</b>	19.2±3.4	18.6±3.3	0.18 (-0.47 to 0.82)	0.517	-1.03% (-1.35 to -0.71)	18.8±2.3	-0.08 (-0.64 to 0.48)	0.568
<b>SLCMJ RSI Mod</b>	0.24±0.07	0.24±0.06	-0.03 (-0.67 to 0.61)	0.900	10.7% (7.38 to 14.02)	0.24±0.05	0.10 (-0.46 to 0.66)	0.987
<b>SLCMJ Peak Power Rel (W/Kg)</b>	32.7±4.4	33.0±3.9	0.17 (-0.47 to 0.82)	0.232	6.01% (4.15 to 7.87)	31.9±4.2	0.25 (-0.31 to 0.82)	0.385

286 PT (peak torque), Rel (relative to body mass), N (Newtons), m (meters), kg (kilograms), W  
287 (Watts), cm (centimeters)

288 **Table 4** Isokinetic and single leg countermovement jump (SLCMJ) results of the involved limb  
289 of the injured group and healthy matched controls

Test	Group 1 Pre-Injury (n=20)	Group 1 Post-Injury (n=20)	PRE vs POST effect size (95%CI)	PRE vs POST P value	Pre-Post Percentage difference (95%CI)	Group 2: Healthy Controls (n=35)	Post-injury vs controls effect size (95%CI)	Post-injury vs controls P value
	Involved limb	Involved limb						
<b>Quad PT Rel (N.m.kg<sup>-1</sup>)</b>	3.2±0.37	2.98±0.51	0.48 (-0.17 to 1.13)	0.036	-7% (-9.2 to -4.8)	3.06±0.4	-0.18 (-0.74 to 0.39)	0.993
<b>HS PT Rel (N.m.kg<sup>-1</sup>)</b>	1.75±0.26	1.96±0.19	-0.90 (-1.58 to -0.23)	<b>≤0.0001</b>	14.2% (9.8 to 18.6)	1.68±0.22	1.32 (0.70 to 1.93)	<b>≤0.0001</b>
<b>SLCMJ Jump Height (cm)</b>	18.5±4.4	14.6±2.9	1.03 (0.34 to 1.71)	<b>0.005</b>	-12.08% (-16.54 to -9.06)	18.8±2.3	-1.64 (-2.28 to -0.99)	<b>≤0.0001</b>
<b>SLCMJ RSI Mod</b>	0.22±0.08	0.18±0.06	0.50 (-0.16 to 1.15)	0.099	-5.04% (-6.6 to -3.48)	0.24±0.05	-0.93 (-1.52 to -0.34)	<b>0.004</b>
<b>SLCMJ Peak Power Rel (W/Kg)</b>	31.7±4.3	30.2±7	0.25 (-0.39 to 0.90)	0.411	-3.14% (-3.61 to -2.67)	31.9±4.2	-0.31 (-0.88 to 0.25)	.325

290 PT (peak torque), Rel (relative to body mass), N (Newtons), m (meters), kg (kilograms), W  
 291 (Watts), cm (centimeters)

292 **Table 5** Countermovement Jump test results of each group

Test	Group 1 Pre- Injury (n=20)	Group 1 Post- Injury (n=20)	PRE vs POST effect size (95%CI)	PRE vs POST P value	Pre-Post Percentage difference (95%CI)	Group 2: Healthy Controls (n=35)	Post- injury vs controls effect size (95%CI)	Post- injury vs controls P value
<b>CMJ Jump Height (cm)</b>	36.4±7.4	33.2±3.7	0.54 (-0.12 to 1.19)	0.042	-5.92% (- 7.76 to - 4.08)	37.5±3.6	-1.17 (- 1.77 to - 0.56)	≤ <b>0.0001</b>
<b>CMJ RSI Mod</b>	0.46±0.11	0.42±0.09	0.39 (-0.26 to 1.04)	0.083	-5.51% (- 7.22 to - 3.8)	0.49±0.07	-0.89 (- 1.48 to - 0.30)	<b>0.001</b>
<b>CMJ Peak Power Rel (W/Kg)</b>	52.1±6.3	49.1±4.6	0.53 (-0.12 to 1.19)	0.042	-4.94% (- 6.47 to - 3.41)	52.8±4.9	-0.76 (- 1.34 to - 0.18)	<b>0.008</b>

293 W (Watts), cm (centimeters), kg (kilograms)

294

295 **Part 2: the effect of ACL reconstruction on the uninjured limb**

296 Uninvolved limb pre-injury and post ACLR performance for each of the participants is shown  
 297 in figures 2b, 3b and 4b). There was no significant main effect of time ( $F(1,19) = 0.43, p =$   
 298  $0.838$ ), but there was a significant main effect of injury on normalised quadriceps peak torque  
 299 ( $F(1,19) = 7.996, p = 0.011$ ). A significant interaction effect between time and injury was  
 300 present ( $F(1,19) = 32.8, p \leq 0.001$ ), showing an increase in normalised quadriceps peak torque  
 301 in the uninvolved limb. No main effect of injury was observed for normalised hamstring peak  
 302 torque ( $F(1,19) = 0.47, p = 0.5$ ) and no significant interaction effect between time and injury  
 303 ( $F(1,19) = 3.8, p = 0.065$ ). There was only a significant main effect of time on normalised  
 304 hamstring peak torque ( $F(1,19) = 7.35, p = 0.014$ ), which showed improvements in normalised  
 305 hamstring peak torque in the uninvolved limb attributable to the passage of time only following  
 306 surgery.

307 There were no significant main or interaction effects of time and/or injury on SLCMJ jump  
 308 height, relative peak power and RSI Mod in the uninvolved limb.

309 Moderate effect size differences in normalised quadriceps peak torque were observed post ACL  
310 reconstruction in comparison to pre-injury values ( $g = 0.57$ , 95%CI [-0.08, 1.23];  $p \leq 0.021$ ),  
311 whereas there were no significant differences in normalised hamstring peak torque (Table 3).

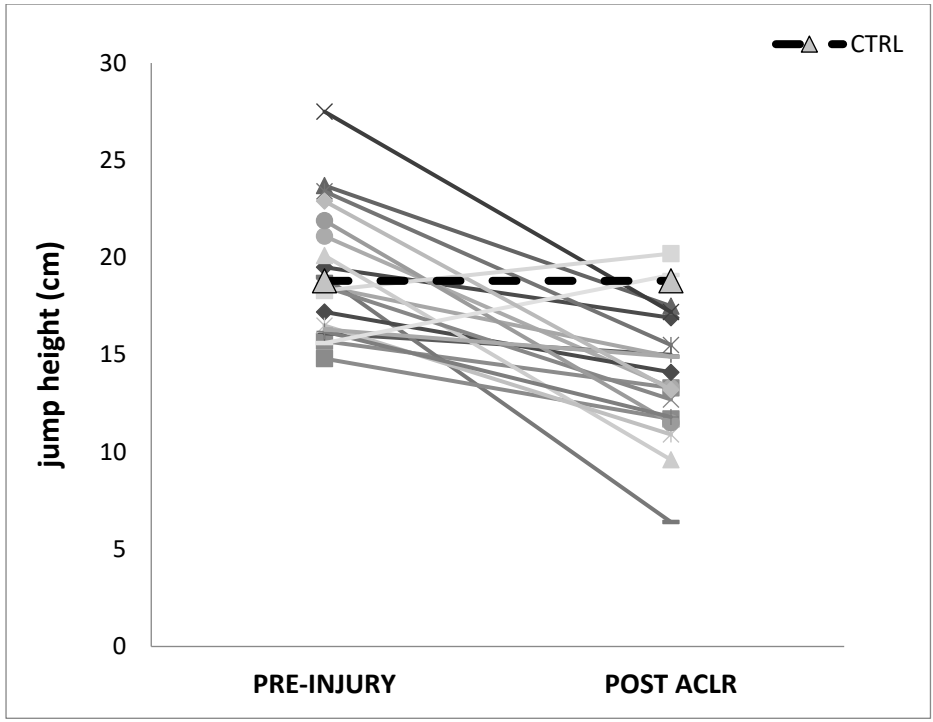
### 312 **Part 3: the effect of ACL reconstruction on the injured limb**

313 Involved limb pre-injury and post ACLR performance for each of the participants is shown in  
314 figures 2a, 3a and 4a. There was no significant main effect of time ( $F(1,19) = 0.43$ ,  $p = 0.838$ ),  
315 but there was a significant main effect of injury on normalised quadriceps peak torque ( $F(1,19)$   
316  $= 7.996$ ,  $p = 0.011$ ). A significant interaction effect between time and injury was present  
317 ( $F(1,19) = 32.8$ ,  $p \leq 0.001$ ), showing deterioration in normalised quadriceps peak torque in the  
318 ACL reconstructed limb. No main effect of injury was observed for normalised hamstring peak  
319 torque ( $F(1,19) = 0.47$ ,  $p = 0.5$ ) and there was no significant interaction effect between time  
320 and injury ( $F(1,19) = 3.8$ ,  $p = 0.065$ ). A significant main effect of time on normalised hamstring  
321 peak torque ( $F(1,19) = 7.35$ ,  $p = 0.014$ ) was shown, which indicates improvements in  
322 normalised hamstring peak torque in the ACL reconstructed limb following surgery.

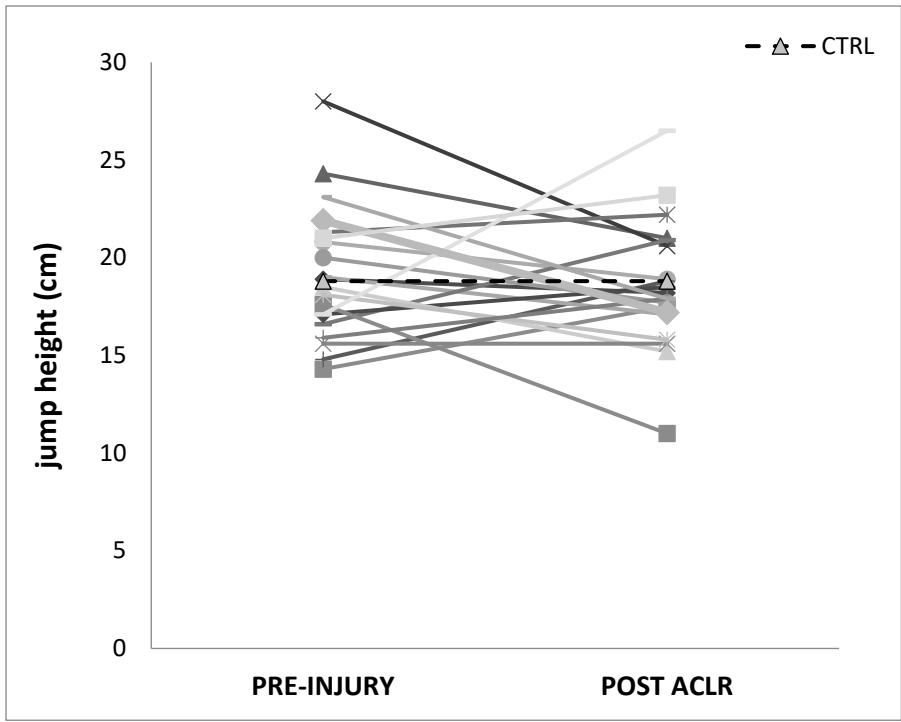
323 There was a significant main effect of time ( $F(1,19) = 5.28$ ,  $p = 0.033$ ) and injury ( $F(1,19) =$   
324  $49.56$ ,  $p \leq 0.001$ ) on SLCMJ height, relative peak power ( $F(1,19) = 31.75$ ,  $p \leq 0.001$ ), and  
325 RSI<sub>mod</sub> ( $F(1,19) = 45.42$ ,  $p \leq 0.001$ ) in the ACL reconstructed limb. A significant interaction  
326 effect was present between time and injury in jump height ( $F(1,19) = 11.53$ ,  $p = 0.003$ ), relative  
327 peak power ( $F(1,19) = 5.86$ ,  $p = 0.026$ ), and RSI<sub>mod</sub> ( $F(1,19) = 8.02$ ,  $p = 0.011$ ), indicating  
328 SLCMJ performance had not returned to baseline. Conversely, normalised hamstring peak  
329 torque was significantly higher following ACL reconstruction compared to pre-injury values  
330 ( $g = 0.90$ , 95%CI [0.23, 1.58];  $p \leq 0.0001$ ). No significant differences in normalised quadriceps  
331 peak torque were present (Table 4).

332

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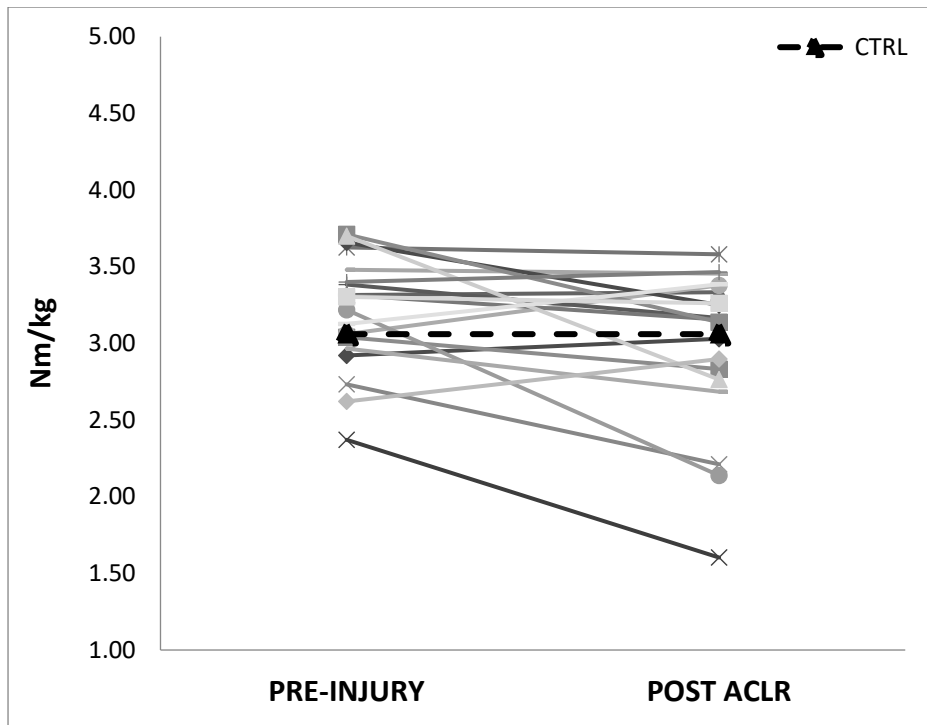


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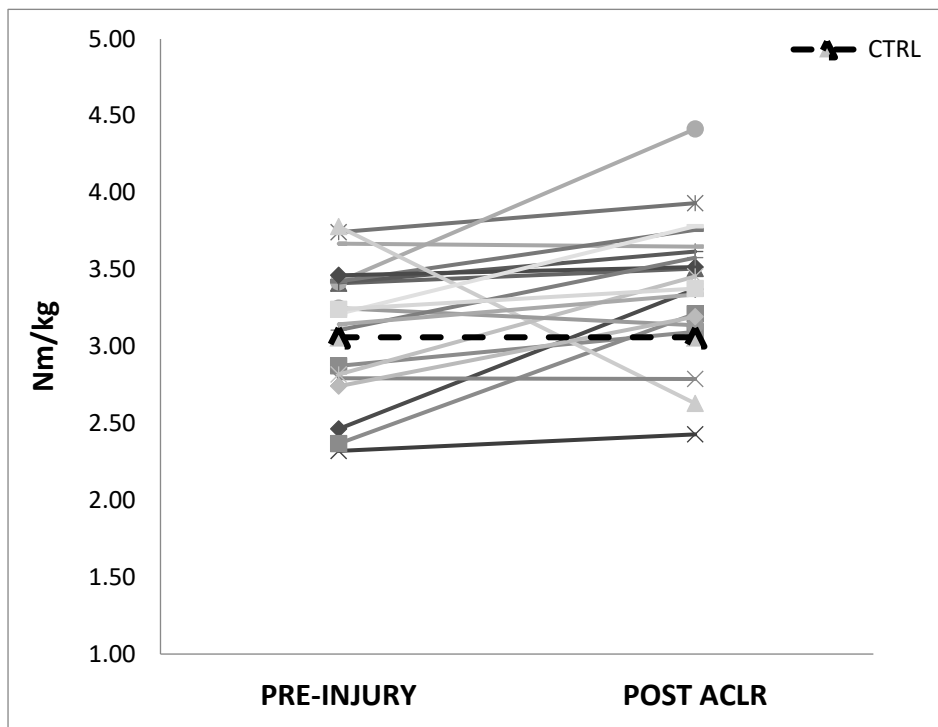
336 **Figure 2a** Involved limb and **Figure 2b** uninvolved limb single leg countermovement jump  
 337 (SLCMJ) height pre-injury and post anterior cruciate ligament reconstruction (ACLR).  
 338 Centimeters (cm). Control group (CTRL)

339





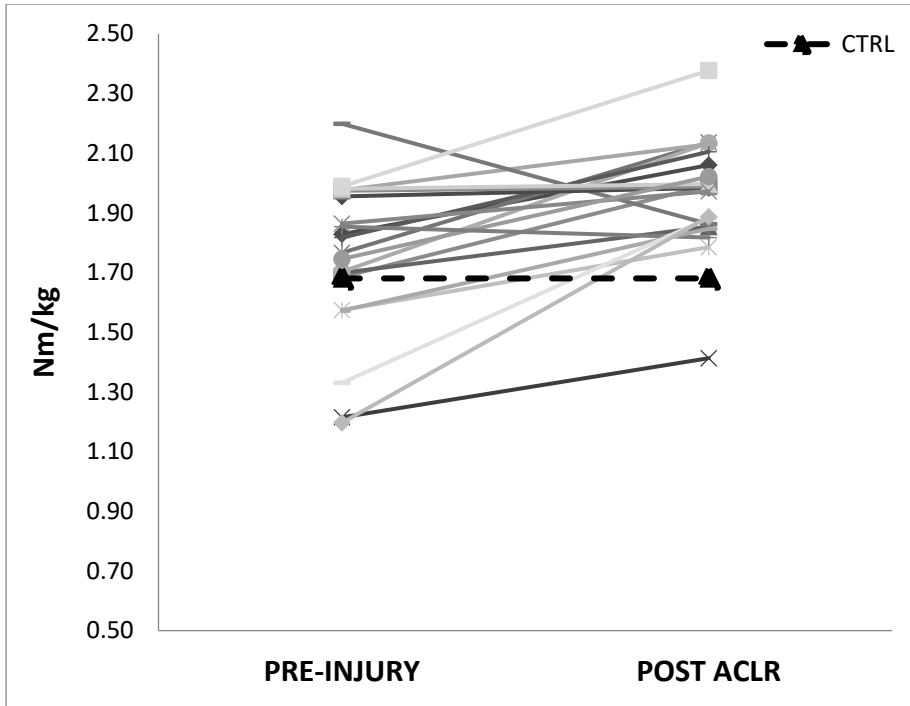
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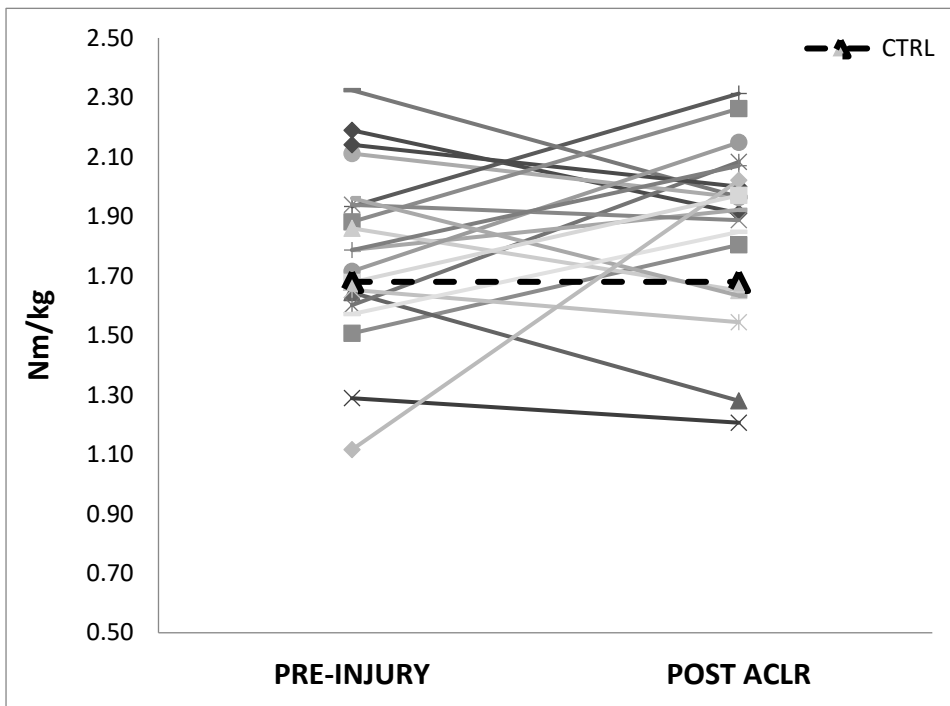
341

342 **Figure 3a** Involved limb and **Figure 3b** uninvolved limb knee extension strength pre-injury  
 343 and post anterior cruciate ligament reconstruction (ACLR). Newton (N). Meter (m). Kilogram  
 344 (kg). Control group (CTRL)

345



346



347

348 **Figure 4a** Involved limb and **Figure 4b** uninvolved limb knee flexion strength pre-injury and  
 349 post anterior cruciate ligament reconstruction (ACLR). Newton (N). Meter (m). Kilogram (kg).  
 350 Control group (CTRL)

351

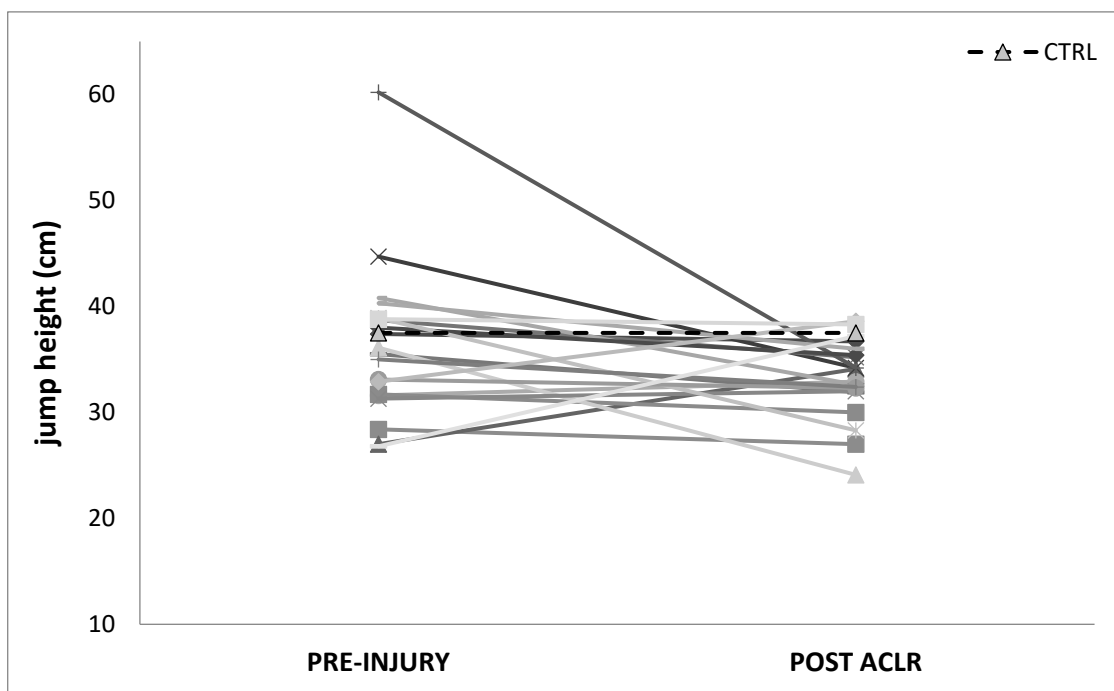
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353

354 **Part 4: the effect of ACL reconstruction on CMJ performance**

355 Pre-injury and post ACLR CMJ height for each of the participants is shown in figure 5. No  
356 significant reductions in CMJ RSImod were present between the ACL reconstructed group  
357 before ACL rupture and after reconstruction at the time of RTS. Although not achieving our  
358 determined alpha level, moderate differences in CMJ jump height ( $g = 0.54$ , 95%CI [-0.12,  
359 1.19];  $p = 0.042$ ) and relative peak power ( $g = 0.53$ , 95%CI [-0.12, 1.19];  $p = 0.042$ ) were  
360 present between the ACL reconstructed group before injury and after reconstruction at the end  
361 of rehabilitation around at the time of RTS (Table 5).

362

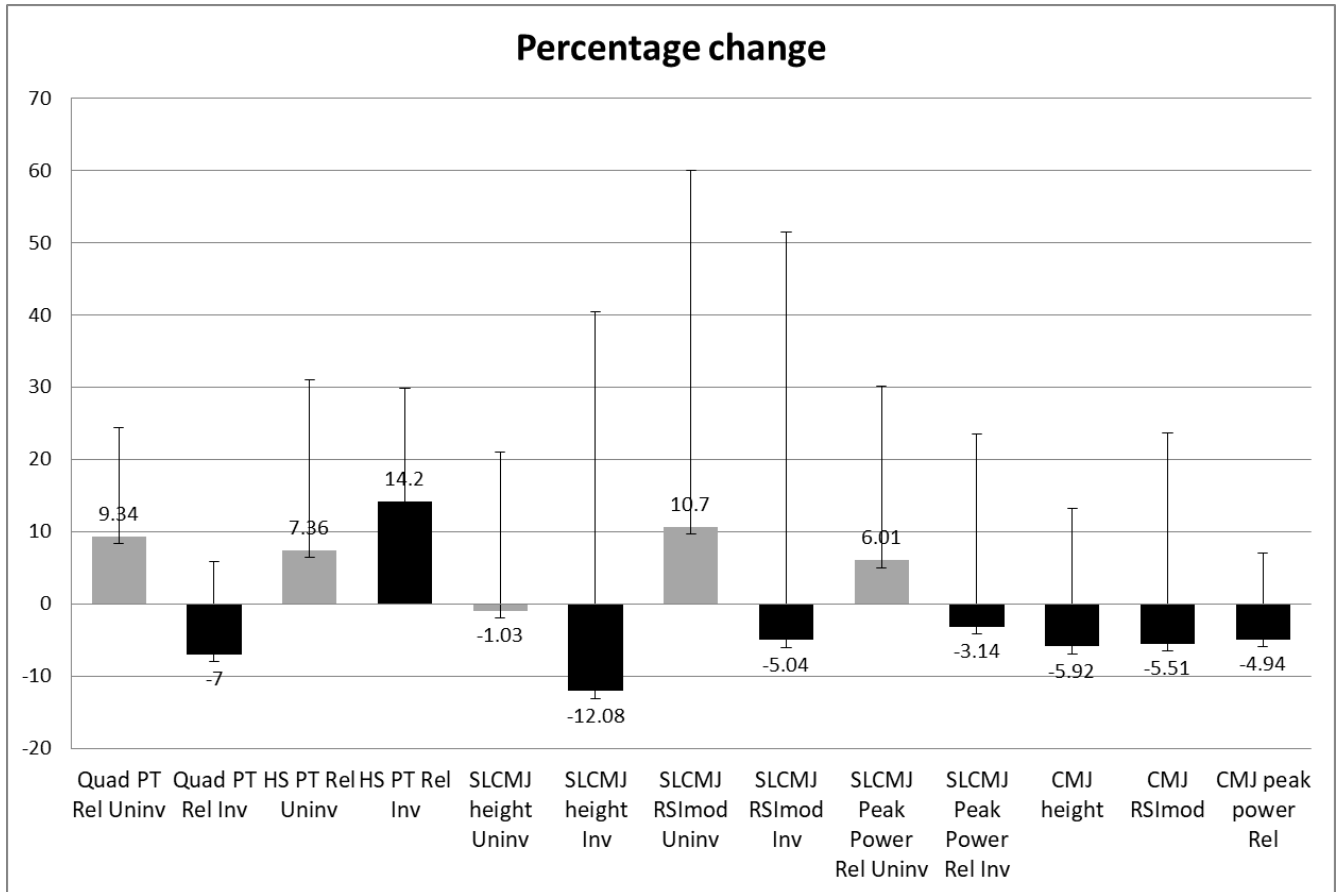


363

364 **Figure 5** Countermovement jump (CMJ) height pre-injury and post anterior cruciate ligament  
365 reconstruction (ACLR). Centimeters (cm). Control group (CTRL)

366

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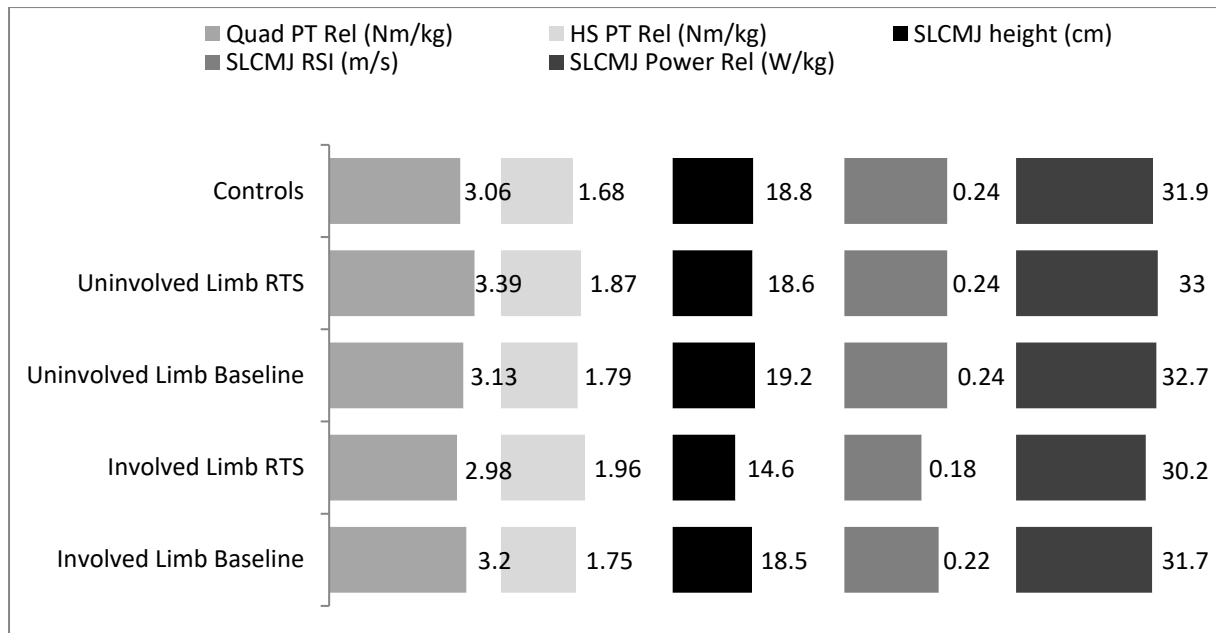


368

369 **Figure 6** Percentage changes from pre-injury to post anterior cruciate ligament reconstruction  
 370 of all variables analysed. Quadriceps relative peak torque (Quad PT Rel), Hamstrings relative  
 371 peak torque (HS PT Rel), single leg countermovement jump (SLCMJ), reactive strength index  
 372 modified (RSImod), relative peak power (peak power Rel), countermovement jump (CMJ),  
 373 uninjured (Uninv), injured (Inv)

374

375



376

377 **Figure 7** Knee extension and flexion strength, single leg countermovement jump height, RSI  
 378 and relative peak power. Newton (N). Meter (m). Centimetre (cm). Metre (m). Second (s).  
 379 Kilogram (kg). Watt (W). RTS (return to sport)

380

## 381 **DISCUSSION**

382 Our aim was to examine how pre-injury data can be used to guide performance recovery and  
383 inform physical readiness as part of RTS decision making. Cumulatively, the results indicate  
384 that residual deficits in strength and power are present following ACL reconstruction ( $7.6 \pm$   
385  $1.8$  months post-surgery) and the pattern of recovery is diverse across tests and metrics  
386 selected. Use of both the uninvolved limb and normative data of matched controls as a proxy  
387 measure to determine the level of performance recovery may not always be appropriate to  
388 estimate the degree of recovery and practitioners are encouraged to collect routine pre-injury  
389 data where possible to most accurately assess physical readiness to RTS.

### 390 *Recovery of involved limb and bilateral performance*

391 Deficits in knee extension peak torque relative to controls have been documented in male  
392 multidirectional team sport athletes more than 6 months following surgery <sup>29</sup>. In our study,  
393 group mean values indicated normalised quadriceps strength levels in the ACL cohort at the  
394 time of RTS were in line with recommended thresholds ( $> 3.0$  Nm/kg at  $60^\circ/\text{s}$ ) <sup>43</sup>, and did not  
395 significantly differ from the uninjured group indicating this should be the first rehabilitation  
396 target. However, there was some variability across participants (figure 3a), and normalised  
397 quadriceps strength of the involved limb post ACL reconstruction showed reduced values  
398 compared to those recorded pre-injury ( $g = -0.48, p = 0.036$ ), suggesting that comparison with  
399 pre-injury values may add important information regarding strength recovery following ACL  
400 reconstruction. Our professional athletes completed a progressive strength training intervention  
401 during rehabilitation which has been shown to attenuate strength deficits following ACL  
402 rehabilitation <sup>43</sup>. However, normalised quadriceps strength on the involved limb was reduced  
403 compared to baseline values and substantially lower than the contralateral limb at the the end  
404 of rehabilitation. These data indicate that both individual limb torque scores need to be  
405 considered in RTS decision making, and when pre-injury data are available, assessment of  
406 symmetry may be secondary compared to attainment of the athletes own benchmark scores on  
407 each limb. Longer rehabilitation periods ( $\geq 9$  months) may also be needed to recover knee  
408 extensor torque deficits <sup>3</sup>. Optimal knee extension strength recovery is associated with reduced  
409 risk of future knee injury <sup>12</sup> and osteoarthritis <sup>9</sup>, greater subjective knee functional scores  
410 (IKDC) <sup>6</sup>, articular cartilage status <sup>11</sup>, and reduced inter-limb and intralimb maladaptive  
411 compensation strategies during unilateral and bilateral jumping and landing tasks <sup>28</sup>. Targeted

412 interventions with a maximal strength emphasis should be integral components of  
413 rehabilitation until at the very least normative values ( $>3.0$  Nm/Kg) are met.

414 Our study revealed a significant reduction in CMJ height, RSImod and relative peak power in  
415 ACL reconstructed players in comparison to baseline pre-injury performance (CMJ height  $g =$   
416  $-0.54$ ,  $p = 0.042$ ; RSImod  $g = -0.39$ ,  $p = 0.083$ ; relative peak power  $g = -0.53$ ,  $p = 0.042$ ) and  
417 healthy controls (CMJ height  $g = -1.17$ ,  $p \leq 0.0001$ ; RSImod  $g = -0.89$ ,  $p = 0.001$ ; relative  
418 peak power  $g = -0.76$ ,  $p = 0.008$ ). For some individuals, CMJ height was substantially lower  
419 than their pre-injury baseline (Figure 5). Other researchers have suggested that recovery of  
420 CMJ height is still incomplete at the time to RTS in comparison to healthy controls<sup>35</sup>. There  
421 was also evidence of large reductions in SLCMJ height ( $g = -1.64$ ,  $p \leq 0.0001$ ) and RSImod ( $g =$   
422  $-0.93$ ,  $p = 0.004$ ) on the involved limb, and this trend was consistent across most participants  
423 (Figure 2a). To execute a single leg jump, there is a higher relative force requirement compared  
424 to bilateral (estimated  $\sim 1.62$  times of those in a CMJ) to displace body mass vertically,  
425 resulting in slower movement velocities<sup>7</sup>. We observed a greater reduction in SLCMJ ( $-$   
426  $12.08\%$ , than CMJ height ( $-5.92\%$ ) following ACL reconstruction (figure 6). Therefore, as the  
427 deficits in SLCMJ height were twice the magnitude of those in the CMJ, it could be suggested  
428 that SLCMJ height offers a better reflection of limb capacity compared to measurement of the  
429 same variable in a bilateral jump. The CMJ task allows athletes to re-distribute their impulse  
430 production via inter-limb compensations in an attempt to maintain similar jump heights<sup>35</sup>.  
431 These data can be derived from dual force platforms but such technology is not commonly  
432 available to clinicians. Measurement of SLCMJ height is obtainable using a variety  
433 measurement tools and may be a useful indicator to determine the recovery of limb capacity  
434 around the time of RTS.

435 Previous research has reported SLCMJ normative scores of  $> 17$  cm in multidirectional field  
436 sport athletes at the late stages of rehabilitation<sup>32</sup>. These values are in line with the results of  
437 our study (figure 7) which included healthy professional soccer players. Therefore,  $\sim 18$  cm  
438 may represent a realistic target to achieve by the end of rehabilitation for field sport athletes if  
439 pre-injury values are not available. However, as many athletes baseline scores were higher  
440 (figure 2a), this further highlights the importance of routine pre-injury data collection at regular  
441 intervals to ensure the most accurate benchmark is established. In addition, the ACL  
442 reconstructed limb showed reduced RSImod in comparison to the dominant limb of healthy  
443 controls (figure 7). Decreased stretch shortening cycle performance has been recently  
444 documented in similar cohorts<sup>19,27,34</sup> and is associated with higher risk of ipsilateral and

445 contralateral ACL injury <sup>17,18</sup>, as well as reduced sports performance <sup>25,30</sup>. Thus, increased  
446 emphasis on reconditioning strategies to recover ballistic performance needs to be embedded  
447 in the RTS pathway together with progressive strength training interventions <sup>4,5</sup>.

#### 448 *The use of proxy measures in decision making*

449 When making RTS decisions, comparison with preinjury is often impracticable. Our data  
450 suggest that in single leg jumping tasks, healthy matched controls including mean values for  
451 team mates or published data for a similar playing level could provide a suitable reference of  
452 the minimum target which should be achieved in monitoring the recovery of physical  
453 performance following ACL reconstruction. However, utilisation of strength scores in healthy  
454 controls may not follow the same pattern. Overestimation of functional improvements during  
455 rehabilitation have been reported previously when using pre-operative scores on the  
456 contralateral limb as a reference value at the time of RTS owing to a bilateral reduction in  
457 physical performance following ACL reconstruction <sup>44</sup> inflating limb symmetry indexes. In  
458 contrast, we observed that normalised quadriceps and hamstring strength improved from pre-  
459 injury following the completion of rehabilitation on the uninvolved limb in the ACL  
460 reconstructed group and scores were greater than matched controls (figure 7) suggesting an  
461 underestimation in the degree of recovery if the latter comparison was used. Conversely,  
462 involved limb reductions in quadriceps strength at the time of RTS were greater when  
463 compared to pre-injury data (7%) and healthy controls (2.6%) suggesting use of healthy control  
464 values would overestimate the degree of recovery for involved limb quadriceps strength. If the  
465 contralateral limb was used post injury, a larger between-limb difference was present (14%)  
466 and this would underestimate the degree of recovery. Our participants were full-time athletes  
467 attending rehabilitation 5 days per week, of which, knee extension and flexion strength were  
468 considered a priority. This suggests that when a comprehensive rehabilitation programme  
469 including progressive strength training is followed, comparison with matched controls alone is  
470 not enough, although it does represent the first achievable milestone to ensure strength  
471 recovery. However, it should be considered that training age and routine exposure to strength  
472 and conditioning of the healthy controls were not examined. Similarly, use of the contralateral  
473 limb may be misleading and can underestimate recovery when significant training adaptations  
474 have occurred. Thus, proxy measures to determine the level of performance recovery may not  
475 always be appropriate.



476 Large performance reductions were observed in bilateral CMJ height and RSImod based on  
477 healthy controls values, but the corresponding deficits based on true benchmark values were  
478 classified as moderate, suggesting a potential underestimation of recovery of these metrics  
479 when using healthy control data. SLCMJ performance on the uninvolved limb showed no  
480 significant difference pre-injury vs. RTS although there was a slight reduction in jump height.  
481 Our data indicate that both healthy controls and the unaffected limb could be used as a  
482 references in monitoring SLCMJ performance recovery (i.e., achievement of pre-injury  
483 baseline values) on a group level, but caution should be applied as several athletes pre-injury  
484 SLCMJ scores were greater than these values.

485 Our data also suggests that a comprehensive rehabilitation program can mitigate reductions in  
486 contralateral knee strength and power secondary to surgery and reduced load exposure.  
487 Maintaining or even increasing quadriceps and plyometric qualities can have important  
488 implications in reducing subsequent ACL injury risk to the uninjured limb in male athletes  
489 following ACL reconstruction<sup>18</sup>, and thus should be monitored during rehabilitation. Further  
490 research is encouraged to measure temporal recovery across multiple timepoints in these  
491 physical qualities to more accurately determine the trajectory of recovery.

#### 492 ***Limitations***

493 Changes from baseline pre-injury scores following ACL reconstruction should be interpreted  
494 relative to the measurement error in the metrics used (Table 1). CMJ height and relative peak  
495 power displayed CV values of 2.7 and 2.1% respectively. The corresponding % changes  
496 following ACL reconstruction and rehabilitation were 5.92 and 4.94% indicating a  
497 ‘real’ change had occurred with differences larger than the observed measurement error.  
498 RSImod reduced by 5.51% but the CV value was 8.6% which suggests the observed differences  
499 were within the error range and could be considered less meaningful. Similarly, only SLCMJ  
500 height showed changes following ACL reconstruction larger than the measurement error (-12%  
501 reduction; CV: 5.2%), whereas RSImod and relative peak power had a greater CV% relative  
502 to the observed % change. In addition, we were not able to collect follow up data on the  
503 uninjured controls to determine what is ‘normal’ seasonal variation in these metrics.

504 Our sample size precluded us from conducting analysis based on graft type and this may have  
505 an effect on strength and power qualities. The majority of our players had a bone-patellar  
506 tendon-bone graft, which can explain the incomplete and delayed recovery of knee extensor  
507 and concentric jump outputs deficits, in comparison to similar cohorts with a

508 semitendinosus/gracilis graft type<sup>31</sup>. Future research may wish to examine temporal recovery  
509 of physical qualities using benchmark pre-injury data considering different graft types. Finally,  
510 none of the assessments directly assessed eccentric qualities, which may show divergent  
511 recovery patterns and deficits, and therefore our conclusions should be considered to be  
512 principally related to concentric strength / jump outputs that ultimately reflect capacity to  
513 generate concentric impulse. Our data were limited to adult male professional football players.  
514 Therefore, generalisation of these results to pediatric, adolescent and female athletes requires  
515 caution. Although the involved surgeons and rehabilitation specialists belonged to the same  
516 Orthopaedic and Sports Medicine Hospital, potential variations in surgical techniques and  
517 rehabilitation strategies could have been present and should also be acknowledged.

## 518 **CONCLUSION**

519 The current study indicates that ACL reconstruction has a detrimental effect on strength and  
520 power characteristics in professional soccer players but the pattern was diverse. Peak knee  
521 extension strength, CMJ and SLCMJ height, RSI<sub>mod</sub>, and relative peak power values at the  
522 end of rehabilitation prior to RTS remained below those recorded pre-injury. Furthermore,  
523 in spite of the fact that players approached strength values deemed sufficient in the ACL  
524 reconstructed limb and exceeded these criteria in the contralateral limb, large differences in  
525 SLCMJ height and RSI<sub>mod</sub> were still evident on the ACL reconstructed limb in comparison to  
526 uninjured matched controls. These differences were smaller when assessed bilaterally (i.e.,  
527 CMJ test), indicating that SLCMJ can be used to more closely evaluate the recovery of  
528 individual limb physical capacity. These data can be easily obtained using a variety of cost  
529 effective methods, especially compared to isokinetic assessments which require expensive  
530 equipment and are time in-efficient.

531 Our findings are summarised in table 6, and have clinical implications to help guide the RTS  
532 process. Cumulatively, we suggest that an optimal approach to determine physical recovery at  
533 the time of RTS would include the following: 1) data collected as early as possible (baseline  
534 pre-injury if available or if not pre-operative values on the uninvolved limb) to inform readiness  
535 to RTS as this should be considered the gold standard reducing the need for proxy measures of  
536 limb recovery, which can overestimate or underestimate limb function; 2) consider both  
537 absolute scores on each limb and not just symmetry values; 3) in situations where baseline pre-  
538 injury data are not available, compare to uninjured matched controls to ensure minimum  
539 standards are met. In addition, we suggest to include both unilateral and bilateral assessments

540 with a range of demands across the strength, power and velocity spectrum to ensure  
 541 performance is measured under different task constraints.

542

Research question	Significant findings
Do the strength and power characteristics differ in soccer players who sustained an ACL injury and underwent subsequent reconstructive surgery to those of uninjured players?	No difference between groups in strength, power and reactive strength characteristics at baseline assessment, but lower performance was indicated in ACL reconstructed players at the end of rehabilitation
How does ACL reconstruction effect isokinetic knee extension / flexion strength and SLCMJ performance on the <i>un-involved limb</i> ?	Increase in quadriceps and hamstring strength from pre-injury to RTS.  No significant differences from pre-injury in SLCMJ height, power and reactive strength following ACL reconstruction
How does ACL reconstruction effect isokinetic knee extension / flexion strength and SLCMJ performance on the <i>involved limb</i> ?	Increase in hamstring strength from pre-injury to RTS  Decrease in quadriceps strength, SLCMJ height and reactive strength following ACL reconstruction
How does ACL reconstruction effect <i>CMJ performance</i> ?	Decrease in jump height, reactive strength and power following ACL reconstruction

543

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671 **Figure 1** Schematic representation of the study design. Uninjured players (black). Injured  
672 players (grey).

673 **Figure 2a** Involved limb and **Figure 2b** uninvolved limb single leg countermovement jump  
674 (SLCMJ) height pre-injury and post anterior cruciate ligament reconstruction (ACLR).  
675 Centimeters (cm). Control group (CTRL)

676 **Figure 3a** Involved limb and **Figure 3b** uninvolved limb knee extension strength pre-injury  
677 and post anterior cruciate ligament reconstruction (ACLR). Newton (N). Meter (m). Kilogram  
678 (kg). Control group (CTRL)

679 **Figure 4a** Involved limb and **Figure 4b** uninvolved limb knee flexion strength pre-injury and  
680 post anterior cruciate ligament reconstruction (ACLR). Newton (N). Meter (m). Kilogram (kg).  
681 Control group (CTRL)

682 **Figure 5** Countermovement jump (CMJ) height pre-injury and post anterior cruciate ligament  
683 reconstruction (ACLR). Centimeters (cm). Control group (CTRL)

684 **Figure 6** Percentage changes from pre-injury to post anterior cruciate ligament reconstruction  
685 of all variables analysed. Quadriceps relative peak torque (Quad PT Rel), Hamstrings relative  
686 peak torque (HS PT Rel), single leg countermovement jump (SLCMJ), reactive strength index  
687 modified (RSImod), relative peak power (peak power Rel), countermovement jump (CMJ),  
688 uninvolved (Uninv), involved (Inv)

689 **Figure 7** Knee extension and flexion strength, single leg countermovement jump height, RSI  
690 and relative peak power. Newton (N). Meter (m). Centimetre (cm). Metre (m). Second (s).  
691 Kilogram (kg). Watt (W). RTS (return to sport)

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