De-Epithelialization Protocol with Tapered Sodium Dodecyl Sulfate Concentrations Enhances Short-Term Chondrocyte Survival in Porcine Chimeric Tracheal Allografts

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Abstract

Background: Tracheal transplantation is indicated in patients with extensive defects that are unable to be repaired via primary reconstruction. However, transplantation is currently considered a high-risk treatment option partly due to high morbidity and mortality associated with graft rejection. Recently, decellularization (decell) has been explored as a technique for creating bioengineered tracheal grafts. However, this method increases risk of post-operative stenosis due to the death of chondrocytes, which are critical to maintain the biochemical and mechanical integrity of tracheal cartilage. In this project, we propose a novel decell protocol that adequately removes epithelial, mucosal, and submucosal cells while maintaining a greater proportion of viable chondrocytes. **Methods:** The trachea of adult male outbred Yorkshire pigs were extracted, decontaminated, and decellularized according to the original and new protocols before incubation at 37 °C in Dulbecco's Modified Eagle Medium (DMEM) for 10 days. Chondrocyte viability was quantified immediately following post-decellularization and on days 1, 4, 7, and 10. Histology was performed pre-decell, post-decell, and post-incubation. **Results:** The new protocol showed a significant (p < 0.05) increase in chondrocyte viability up to four days after decell when compared to the original protocol. The new protocol also preserves extracellular matrix (ECM) composition to a similar degree as the original protocol. **Conclusion:** Despite limited improvements in long-term chondrocyte viability, the new protocol may be used to engineer chimeric tracheal allografts without the need for cartilage regeneration up to four days post-decellularization.

Key Words: Tissue Engineering; Decellularization; Allograft; Trachea; Bioreactor; Regenerative Medicine; Chondrocyte; Stem Cell; Graft; Transplantation; Transplant; Surgery; Bioengineering; Stenosis; Cartilage; Viability; Cell Viability; Medicine (Source: MeSH-NLM).

Introduction

Tracheal transplantation is a surgical procedure that aims to restore the airway in patients with extensive defects that are unable to be repaired via primary reconstruction. Transplantation is indicated in cases where injury exceeds 50% of the organ in adults and 30% in children.¹ However, tracheal replacement therapy is currently considered a high-risk procedure, and is mostly offered as a treatment option in compassionate use cases. A major reason behind the relatively high rate of complications is the plethora of immunological compatibility issues created by orthotopically transplanting a donor organ.² A possible solution to this problem may be found in tissue engineering-based

approaches for whole-trachea regeneration. Recently, significant progress has been made in engineering bioartificial organs de novo from pluripotent stem cells and acellular extracellular matrix (ECM) scaffolds.^{3–6} Somatic cells have been differentiated into functional lung epithelial cells after transformation into induced pluripotency.⁷ Also, stem cell-seeded tracheal grafts from cadaveric donors have been transplanted into patients with end-stage airway diseases.⁴ Despite these milestones, recellularized tracheal allografts still demonstrate increased risk of stenosis, resulting in post-operative complications.^{3,4,8}

Decellularization (decell) of donor trachea is a relatively wellstudied technique for creating natural scaffolds for whole-trachea

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regeneration.⁹⁻¹⁵ One such decell approach involves the use of detergents to remove donor cells from a cadaveric trachea, leaving behind the ECM scaffold.^{11,16,17} Recipient-derived induced pluripotent stem cells (iPSCs) may then be seeded onto such scaffold, thereby reconstituting the respiratory epithelium.⁴ The benefits of this approach are twofold. Firstly, risk of graft rejection is reduced because the immunogenic donor tracheal epithelium and submucosa are removed and replaced with autologous cells.^{8,10,18-20} Secondly, the use of a native biological scaffold rather than synthetic materials preserves the important tissue architecture and ultrastructure, which allows for greater mimicking of the cellular niche later during scaffold seeding.¹⁷ However, the full thickness decell protocols currently in use are harmful to chondrocytes, leading to deficiencies in the biochemical and mechanical integrity of hyaline cartilage.^{14,17,21} This may increase the risk of post-operative stenosis and other complications upon implantation.²² To address this issue, the Waddell lab uses a de-epithelialization (de-ep) technique pioneered by Aoki et al. in 2019 to remove only the immunogenic epithelium while maintaining chondrocyte viability.^{17,23} This deep technique can be followed by re-epithelialization (re-ep) using autologous cells to produce chimeric tracheal allografts.

Despite these advances, the original de-ep protocol is suboptimal due to relatively low chondrocyte survival rates (68.6 \pm 7.3%).¹⁷ A new de-ep protocol has recently been developed by the Waddell lab based on the postulated chemical and osmotic effects of various decellularization agents on chondrocytes. This protocol is believed to provide milder de-ep conditions that may increase chondrocyte survival while providing similar removal of epithelial cells. When designing this new protocol, the following hypotheses were made: 1) removal of the standard 40 minute ddH2O wash cycle will decrease osmotic stress on cells perforated by sodium dodecyl sulfate (SDS) detergent, the most common decellularization agent used in previous protocols, and 2) using decreasing concentrations of SDS rather than a static concentration will remove greater amounts of residual SDS in submucosal tissue, thus protecting cartilage. An initial high concentration (1%) is required for decellularizing epithelium and mucosa, after which lower concentrations of SDS (0.1%, 0.01%) are more appropriate for minimizing damage to cartilage. This study intends to serve as a proof-of-concept to demonstrate that a modified de-ep protocol can allow the removal of immunogenic tissue (epithelium, mucosa, submucosa, and perichondrium) while preserving a greater portion of the chondrocyte population. The objectives of this study are to: 1) evaluate chondrocyte viability in porcine trachea after the use of the new de-ep protocol, 2) evaluate the preservation of ECM biochemical composition after the new protocol, and 3) evaluate the degree of epithelial cell attachment and viability during re-ep after the new protocol. We hypothesize that the new protocol will produce de-epithelialized scaffolds with improved chondrocyte viability while demonstrating similar biochemical composition and reepithelialization performance as compared to the current protocol.

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Figure 1. **A**: The Perfusion Circuitry Designed for the Original de-ep Protocol.¹⁷ Order of Perfusion is Numbered from 1-4 and Corresponds to the Solutions in Table 1. **B**: The Perfusion Circuitry Designed for the new de-ep Protocol. Order of Perfusion is Numbered from 1-5 and Corresponds to the Solutions in Table 2.

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Methods

Tracheal extraction

Adult male outbred Yorkshire pigs (30-40 kg) (n = 18) sourced from the University Health Network (UHN) Animal Resources Centre were used as donor animals due to the physiological similarity of their cardiopulmonary system to that of humans. After anesthesia by isoflurane administration, a median incision of the neck was made to expose the larynx and upper trachea. Next, a median sternotomy was performed to open the chest wall and provide access to the lower trachea. Using Mayo scissors, the trachea was bisected just below the cricothyroid membrane and lifted away from the esophagus. Surrounding connective tissue was dissected away using curved Mayo scissors. To detach the trachea, the left and right main bronchus were bisected just below the carina. The extracted trachea was immediately placed in decontamination solution at 0 °C until transported out of the operating room. The decontamination solution contained Hank's balanced salt solution (HBSS, ThermoFisher, USA) supplemented with 2% (w/v) bovine serum albumin (BSA, ThermoFisher, USA), fluconazole (4 µg/mL, Gibco, USA), colistimethate (5 µg/mL, Gibco, USA), imipenem/cilastatin (25 µg/mL, Gibco, USA), ceftazidime (154 µg/mL, Gibco, USA), penicillin (200 U/mL, Gibco, USA), streptomycin (200 µg/mL, Gibco, USA), amphotericin B (2.5 µg/mL, Gibco, USA) and gentamicin (50 µg/mL, Gibco, USA). The tracheas were subsequently incubated at room temperature on a rocking platform (30rpm) for 2 hours. After this incubation, the decontamination solution was replaced with fresh solution, and luminal mucus was scraped off using a micro-tapered stainlesssteel spatula. The tracheas were incubated at 4 °C overnight until de-ep was performed the next morning.

Animals selected for tracheal extraction surgery were screened against the following exclusion criteria:

- · Respiratory pathologies,
- Participation in concomitant respiratory studies (ex: bleomycin lung injury model), and
- More than 30 minutes since cardiac death (donor warm ischemia time).

All animals received humane care in compliance with the "Principles of Laboratory Animal Care" formulated by the National Society for Medical Research and the "Guide for the Care of Laboratory Animals" published by the National Institutes of Health. The study was approved by the Animal Care Committee of the Toronto General Research Institute.

De-epithelialization and incubation

The following solutions were prepared under sterile conditions and adjusted to a pH of 7.4: 1%, 0.1%, and 0.01% SDS; 1% triton X-100; Dulbecco's phosphate buffered saline (DPBS). A perfusion system was constructed using polyvinyl chloride (PVC) tubing and 4-way Luer connection stopcocks as illustrated in *Figure 1*. A rotating perfusion bioreactor was used, modified from Haykal et al. Using three 2/0 silk sutures, the trachea was anastomosed to

the bioreactor with its proximal end facing the inlet of the chamber (*Figure 2*).⁴ De-ep was performed according to the original, new, and control protocols outlined in *Tables 1-2*.¹⁷

Table 1. Original de-epithelialization Protocol.¹⁷

Step	Reagents*	Time	Vol. (mL)	рΗ	Temp. (°C)
1+	1% SDS	3 hr	75	7.4	37
2+	ddH_2O	30 min	140	7.4	37
4‡	1% Triton	30 min	140	7.4	37
5‡	DPBS (-/-)	30 min	140	7.4	37

Legend: * Reagents inside trachea (Lumen). Outside the trachea, DMEM with 10% FBS + 1% Penicillin-Streptomycin solution remains circulating.

+ De-epithelialization process - pulsatile perfusion

* Washing steps – continuous perfusion

DMEM = Dulbecco's Modified Eagle Medium

SDS = Sodium Dodecyl Sulfate

DPBS = Dulbecco's Phosphate-Buffered Saline

Following de-ep, the proximal and distal ends of the trachea were trimmed such that only the portions exposed to the decellularization media were used for the subsequent 10-day incubation. The tracheal segments were then placed in decontamination solution for 48 hours at 4 °C on a rocking platform (30 rpm). Finally, the tracheae were incubated at 47 °C with 5% CO2 (ThermoFisher, USA) in a 250 mL Erlenmeyer flask fitted with a 20-micron filter allowing for gas exchange. The media used was Dulbecco's Modified Eagle Medium (DMEM, Gibco, USA) supplemented with 10% (v/v) fetal bovine serum (FBS, Gibco, USA), fluconazole (4 µg/mL), colistimethate (5 µg/mL), imipenem/cilastatin (25 µg/mL, Gibco, USA), ceftazidime (154 µg/mL, Gibco, USA), penicillin (200 µg/mL, Gibco, USA), streptomycin (200 µg/mL, Gibco, USA), amphotericin B (2.5 µg/mL, Gibco, USA) and gentamicin (50 µg/mL, Gibco, USA). Media was changed every 48 hours.

Table 2. New De-Epithelialization Protocol.

Step	Reagents*	Time	Vol. (mL)	рΗ	Temp. (°C)
1†	1% SDS	1 hr	75	7.4	37
2†	0.1% SDS	1 hr	75	7.4	37
3†	0.01% SDS	1 hr	75	7.4	37
4‡	1% Triton	30 min	140	7.4	37
5‡	DPBS (-/-)	30 min	140	7.4	37

Legend: * Reagents inside trachea (Lumen). Outside the trachea, DMEM with 10% FBS + 1% Penicillin-Streptomycin solution remains circulating

+ De-epithelialization process - pulsatile perfusion

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DMEM = Dulbecco's Modified Eagle Medium

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To accurately compare the two de-ep protocols being tested, two negative control groups were employed. The first control was a decontaminated native trachea that immediately underwent static incubation for ten days without any de-ep procedure, henceforth referred to as "control-native." The second control was exposed to the same conditions as the trachea that underwent the new protocol, except with DPBS replacing all steps that required SDS, henceforth referred to as "control-DPBS" (*Table 3*).

Figure 2. Timepoints for live/dead Staining and Histology used in this Study. Bottom left: Appearance of the Bioreactor with lid Removed. Trachea is Visible, Surrounded by Dulbecco's Modified Eagle Medium (DMEM).



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Two control groups are necessary to rule out any potential negative effects on chondrocyte viability arising from tracheal harvesting and installation into the bioreactors. If both controls demonstrate similar levels of near-100% viability, the study can conclude that the primary determinant of chondrocyte viability is the protocol itself, in other words, the series of SDS decellularization steps. Three biological replicates – each consisting of a single trachea harvested from a random Yorkshire pig – were performed for the original protocol, the new protocol, and the two control groups.¹⁷ Day 0 was defined as the start of the bioreactor incubation period, hence day –2 was when the decellularization protocol was performed. *Figure 3* illustrates the study protocol as a flowchart diagram.

Histological analysis

Histological samples were taken from the trachea before de-ep, after de-ep, and after incubation (*Figure 4*). Specimens were fixed with 4% paraformaldehyde for 24 hours and processed with an automated vacuum tissue processor (Leica, USA). Tissue was sectioned into 5 µm slices and stained with hematoxylin and eosin (H&E), Masson's trichrome (Sigma-Aldrich, USA), Verhoeff's elastin (Sigma-Aldrich, USA), and Alcian blue (NovaUltraTM, IHC World, USA).

Figure 3. The Experimental Protocol Followed in the Current Study, Illustrated as a Flowchart Diagram.



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Table 3. Control – New De-Epithelialization Protocol without SDS. Identical Conditions as new Protocol, Except Perfused with DPBS Instead of SDS for Preparation of Control-DPBS Trachea.

Step	Reagents*	Time	Vol. (mL)	рΗ	Temp. (°C)
1†	1% DPBS	1 hr	75	7.4	37
2†	1% DPBS	1 hr	75	7.4	37
3†	1% DPBS	1 hr	75	7.4	37
4‡	1% Triton	30 min	140	7.4	37
5‡	DPBS (-/-)	30 min	140	7.4	37

Legend: * Reagents inside trachea (Lumen). Outside the trachea, DMEM with 10% FBS + 1% Penicillin-Streptomycin solution remains circulating. † Deepithelialization process – pulsatile perfusion. ‡ Washing steps – continuous perfusion. DMEM = Dulbecco's Modified Eagle Medium. SDS = Sodium Dodecyl Sulfate. DPBS = Dulbecco's Phosphate-Buffered Saline

Quantification of chondrocyte viability

Chondrocyte viability was quantified immediately after de-ep and on days 1, 4, 7, and 10 (Figure 3). Two to three rings were obtained from each trachea for a membrane integrity-based viability assay. The mucosa and submucosa were dissected away from the cartilage using fine forceps. The cartilage ring was opened and manually cut in cross section into thin (<1 mm) slices. ethidium homodimer (LIVE/DEAD™ An assav Viability/Cytotoxicity Kit, Invitrogen, USA) was performed as per manufacturer directions. The slices were imaged under confocal microscopy at 20x magnification (A1R, Nikon, Japan). Images were then examined manually by a blinded experimenter. Portions of the image containing viable chondrocytes were circumscribed and the area was calculated. The percentage viability of an image was calculated through the following formula:

% chondrocyte viability =
$$\frac{Area \ of \ viable \ chondrocytes}{Total \ cartilage \ area} \times 100\%$$

Three technical replicates were performed per trachea.

Re-epithelialization

The de-ep bioreactor circuitry from Haykal et al. was modified to include media reservoirs for oxygenation, in addition to syringe ports for media changes and sample collection.⁴ A 1 mL suspension of BEAS-2B human bronchial epithelial cells ($\sim 1 \times 10^6$ cells/cm²) was injected into the lumen. Cells were allowed to adhere for 2 hours under bidirectional flow at a rate of 1.5 mL/min. After the initial 2 hours, we started unidirectional perfusion of the lumen at the same rate for seven days. During re-ep, media in the luminal circuit (30 mL) was changed every 24 hours and media in the outer circuit (250 mL) was changed every 48 hours.

Cell proliferation activity assay

Cell proliferation during re-ep was measured using a resazurinbased cell viability assay as per manufacturer instructions (PrestoBlue®, Invitrogen, USA). Briefly, a 20 mL solution of 1:20 (v/v) PrestoBlue/DMEM + 10% FBS was prepared. Three 0.5 mL volumes were separated for use as a negative control. The remaining 18.5 mL of reagent was injected into the luminal perfusion circuit of the bioreactor and allowed to circulate for 1 hr. Afterwards, the PrestoBlue solution was aspirated out of the luminal circuit and aliquoted into three 0.5 mL replicates in a 24-well plate for fluorescence analysis at 560 nm (CytationTM 5, BioTek Instruments).

Figure 4. Chondrocyte Viability Following De-epithelialization and 10-day Incubation in Static Media. Statistically Significant Differences as Determined by a Two-Way Analysis of Variance (ANOVA) with Tukey's Post Hoc Multiple Comparisons Test are Indicated. P-Values Given as: <0.0332 = *, <0.0021 = **, <0.0002 = ****, <0.0001 = ****



Statistical analysis

Commercial statistical software (GraphPad Software Inc., USA) was used for statistical analysis. A 2-way analysis of variance (ANOVA) was used to determine statistically significant differences ($p \le .05$) between the three protocols (original, new, control-DPBS), with Tukey's post hoc multiple comparisons test. Values in figures are presented as means with standard deviations (SD).¹⁷

Results

Quantification of chondrocyte viability

There exists an overall negative correlation between days since de-ep and percentage chondrocyte viability (Figure 4). Both the original and new protocols significantly reduce viability compared to the control protocol (no SDS) and unprocessed native trachea.¹⁷ However, the new protocol provides significantly (p = 0.0069) improved viability compared to the original protocol in the first four days, after which there is no detectable difference.¹⁷ The most marked improvement in chondrocyte viability occurs on day 4 (61.3±10.8% vs 40.7±5.7%), yet the benefit of the new protocol towards chondrocytes is seen as early as immediately after de-ep on day -2 (78.1±4.7% vs 61.5±10.7%). In other words, long-term chondrocyte survival remains unchanged. Qualitative inspection of live/dead staining reveals the most chondrocyte death at the luminal surface of each cartilage ring (Figure 5). There appears to be a smaller "wavefront" of chondrocyte death in the new protocol compared to the original protocol. The average chondrocyte viability of two replicates (n=2) after a 7-day re-ep was 63%.

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Figure 5. Chondrocyte Viability in new Protocol, Original Protocol, and Control-Native Trachea on day 10 of Static Incubation.¹⁷ Confocal Microscopy Images Depicting Calcein-AM for live (Green) and Ethidium Homodimer-1 for dead (Red) Cells in Cross-Sections of Cartilage Rings (Marked as the area within the White Dotted Line). Bottom Right Image Shows the Calculation for Percentage Viability as the area within the Solid Yellow Line (Live Cells) Divided by area within the White Dotted Line (Total Cross-Sectional Area).



Histological analysis

In the native trachea control, H&E staining showed the expected pseudostratified columnar epithelium with cilia and goblet cells (*Figure 6*). In both the original and new de-ep protocols, H&E showed a denuded epithelium, with no residual cellular material.¹⁷ No nuclei or cytosolic elements were found in the epithelium. However, both protocols resulted in some nuclei remaining in the deep submucosal regions. Residual acinar gland cells were also visible in both protocols. The hyaline cartilage appears morphologically unchanged.

Masson's trichrome stain showed good collagen preservation throughout the ECM in both the original and new protocols (*Figure 6*).¹⁷ Keratin fibers in the deep submucosa appear better preserved in the new protocol. Verhoeff's elastin stain showed good preservation of elastin fibers in the mucosa and submucosa of both the original and new de-ep protocols (*Figure 6*).¹⁷ Alcian blue stain showed good preservation of acidic polysaccharides such as glycosaminoglycans in cartilage, in both the original and new protocols (*Figure 6*).¹⁷ De-Epithelialization Protocol with Tapered Sodium Dodecyl Sulfate Concentrations Enhances Short-Term Chondrocyte Survival in Porcine Chimeric Tracheal Allografts

Figure 6. **A)** Masson's trichrome stain **B)** Verhoeff's elastin stain **C)** Alcian blue stain **D)** Hematoxylin and eosin stain of control-native; trachea processed with the original/current de-ep protocol; and trachea processed with the new de-ep protocol.¹⁷ 10x and 60x magnifications are shown in the top and bottom rows respectively. The lumen (L), epithelium (E), submucosa (SM), acinar glands (AG) and hyaline cartilage (HC) are labelled.



Cell proliferation activity assay

When the new protocol's re-ep cell proliferation curve is compared with that of the original protocol from Aoki et al., there is similarity in the rate at which fluorescence increases (*Figure* D.¹⁷ The difference between the two growth curves is

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nonsignificant (p=0.15, 0.59, 0.86, 0.59, 0.89, 0.20, 0.84) as indicated by a multiple t test (false discovery rate approach). Although not a focus of this study, chondrocyte viability after the 7-day re-ep with BEAS-2B was evaluated with two tracheae. The average chondrocyte viability was 63%.

Figure 7. Growth Curves of BEAS-2B on the New and Old Protocol's Scaffolds over Seven-Day Re-Epithelialization Period.



Legend: p = 0.15, 0.59, 0.86, 0.59, 0.89, 0.20, 0.84.

Discussion

It has been demonstrated in previous literature that SDS reduces cell viability by acting as an anionic detergent, perforating the cell membrane and causing osmotic lysis.^{11,12,22} The original protocol contains a 3 hour 1% SDS wash that can leave residual detergent trapped in tissue, thus causing ongoing damage after the protocol is terminated.¹⁷ Furthermore, the original protocol includes a 30 minute ddH_2O wash that can cause further chondrocyte death via osmotic imbalance leading to cytolysis.¹⁷ The new protocol made two changes to the original protocol: 1) the 3 hour SDS cycle has been replaced with three 1 hour cycles at decreasing SDS concentrations (1%, 0.1%, 0.01%), and 2) The 30 minute ddH₂O wash has been removed.¹⁷ It is believed that the first change limits deep penetration of residual SDS into tissue, while the second change reduces cytolysis of chondrocytes. In other words, this new protocol was designed to provide milder de-ep conditions that increase chondrocyte survival while providing similar removal of epithelial cells. Both negative controls (control-native and control-DPBS) showed close to 90% viability. Therefore, it seems that SDS retention in the ECM is a major contributor to chondrocyte death after de-ep, overshadowing the cytolytic effect of the ddH2O wash and other potential minor contributors. Attempts at quantifying the amount of residual SDS in de-epithelialized tissues using a methylene blue assay were unsuccessful. Future studies should investigate the relationship between residual SDS levels and chondrocyte viability. The short-term nature of the improvement in chondrocyte viability observed in this study was likely due to an initial reduction in residual SDS concentration in submucosal

tissues, followed by eventual permeation of the SDS through submucosa and into cartilage due to passive diffusion. Confocal images of the cell viability assay show a clear delineation between calcein-AM (live cells) and ethidium homodimer-1 (dead cells), suggesting a progressive "wavefront" of cell death that is consistent with diffusion of residual SDS. Confirmation of this theory is required, although preventing the diffusion of SDS through submucosal tissue would be difficult or impractical to accomplish in any de-ep protocol.

Examination of H&E slides shows that both protocols were extremely efficient at denuding the epithelium. However, neither protocol appears to sufficiently decellularize acinar glands. Furthermore, the new protocol seems to be less efficient at decellularizing deep submucosal layers. This result was expected since the new protocol uses decreasing concentrations of SDS and is less aggressive overall compared to the original protocol, among others.^{17,24,25} Therefore, with the current detergent-based methods of de-ep, the goal of selectively preserving chondrocyte viability seems to depend on the careful titration of SDS concentrations, walking a fine balance between over- and under-decellularization. The current study shows that the new protocol sacrifices decellularization performance in return for better chondrocyte survival.

Previous studies have shown that decellularization cycles can reduce several ECM components that are critical to structural integrity, including elastin, collagen, and glycosaminoglycans.17,25,26 Qualitative histological analysis demonstrated that the new protocol is not any more damaging to ECM components than the original protocol.¹⁷ Elastin, collagen, and glycosaminoglycans were found to be preserved after de-ep to a similar degree as with the original protocol.¹⁷ Tracheal compliance and viscoelasticity were not tested because previous studies by Aoki et al. have confirmed no difference in these mechanical properties after the more aggressive original de-ep protocol.17

The cellular proliferation assay suggests that the new protocol has no negative effects on metabolism and growth of the BEAS-2B cells used for re-ep. This suggests that ECM scaffolds created using the new de-ep protocol can support epithelial cell attachment and viability during re-ep, allowing for the creation of chimeric allografts.

This proof-of-concept study is not without limitations. To longitudinally measure chondrocyte survival, we incubated the de-epithelialized trachea in static Dulbecco's Modified Eagle Medium (DMEM) to simulate implantation of the grafts. This does not fully recapitulate the complex cell-environment interactions present in vivo. Therefore, conclusions regarding chondrocyte viability should be validated in a bioreactor environment that simulates nutrient perfusion, hydrodynamic stimuli, and mechanical stimuli.^{27,28} The current study did evaluate chondrocyte viability of de-epithelialized trachea after a 7-day re-

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ep in a double-chamber bioreactor, yielding a percentage viability of 63% over 7-days. This result is promising given that previous studies have demonstrated that a 50% chondrocyte viability was associated with successful tracheal transplantation in dogs, with no lethal stenosis.²⁹ However, future studies should be conducted with a larger number of replicates.

In conclusion, we introduce a new de-ep protocol with improved short-term chondrocyte viability. The results of this study have indicated that improvements in the protocol can still be made. However, the data presented sheds light on the potential mechanism of chondrocyte death during and after de-ep.

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Author Contributions

Conceptualization: KXZ, FGA, GK, SH, TKW. Data Curation: KXZ. Formal Analysis: KXZ. Funding Acquisition: GK, TKW. Investigation: KXZ, FGA, AM. Methodology: KXZ, FGA. Project Administration: KXZ, FGA, GK, SH, TKW. Resources: KXZ. Software: KXZ. Supervision: FGA, AM, GK, SH, TKW. Validation: KXZ, FGA. Visualization: KXZ. Writing - Original Draft: KXZ. Writing - Review Editing: KXZ.

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