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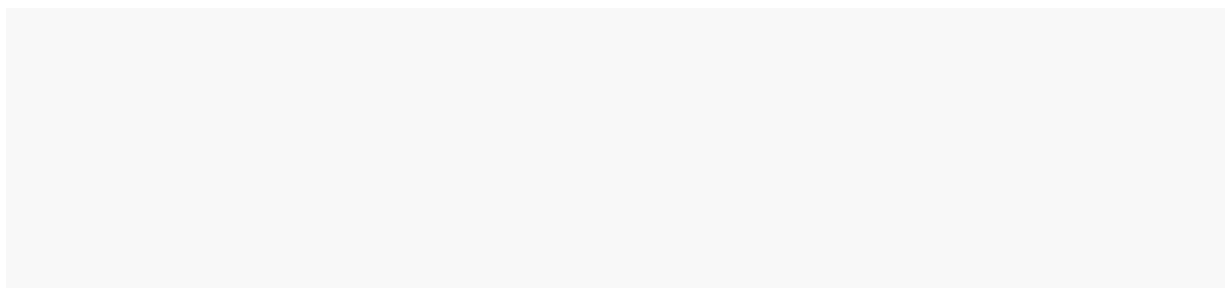
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1 **pH Responsive polyurethane (core) and cellulose acetate phthalate (shell) electrospun fibers**
2 **for intravaginal drug delivery**

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16
17 **Abstract**

18 In this study we present the use of co-axial electrospinning to produce core-shell composite micro-
19 /nano- fibers of Polyurethane (PU) and Cellulose acetate phthalate (CAP). The designed fibers possess
20 enhanced mechanical properties with a tensile strength of 13.27 ± 2.32 MPa, which is a clear
21 improvement over the existing CAP fibers that suffer from a poor mechanical strength (0.2 ± 0.03 MPa).
22 The CAP imparts pH responsiveness to the core-shell structure giving the fibers potential for “semen
23 sensitive” (intravaginal) drug delivery.

24 **Key words:** core-shell electrospinning; cellulose acetate phthalate; polyurethane; intravaginal drug
25 delivery

26 **1. Introduction**

27 In recent years, the acquired immunodeficiency syndrome (AIDS), caused by human
28 immunodeficiency virus (HIV), has become a serious threat to human health. Until now, about 33
29 million people are infected by HIV (Mamo, Moseman et al., 2010). The prevalent sources of
30 transmission of this virus are mainly through sexual contact, transfusion of contaminated blood or
31 medical products such as syringes. The prevention of this pandemic disease has been better than its
32 cure since the HIV virus presents varied genetic variability retarding the development of suitable
33 vaccines. Hence, the most common methods of prevention of this deadly disease have been the use of
34 condoms and microbicides. However, in most of the developing countries, the use of condoms and
35 microbicides has been restricted due to social taboos (Date and Destache, 2013). Clearly, alternate
36 strategies to combat or prevent HIV spreading remain highly needed.

37 In our previous work (Huang, Soenen et al., 2012), we designed cellulose acetate phthalate (CAP)
38 fibers by electrospinning. CAP is being intensively used as pharmaceutical excipient to coat capsules
39 and tablets, with the aim to avoid drug release in the acidic stomach while allowing drug release in the
40 more alkaline intestine. We showed that electrospun CAP-fibers instantaneously dissolve upon contact
41 with (human) semen. Indeed, as the pKa of CAP equals 5.28 (Rando, Obara et al., 2006), it is expected
42 to be minimally soluble in healthy vaginal flora but highly soluble when exposed to semen with a pH
43 of approximately 7. Note that CAP itself has gained attention as well for its anti-HIV effect due to its
44 ability to induce conformational changes in the HIV glycoproteins gp41 and gp120 (Neurath, Strick et
45 al., 2002). We thus suggested that CAP-fibers could have potential for ‘semen triggered’ delivery of
46 (anti-viral) drugs.

47 The previously designed electrospun CAP-fibers showed, however, a (very) poor mechanical

48 performance, resulting in fractures, which would clearly limit their intravaginal use. The current
49 research effort has been dedicated to overcome this drawback through the design of core-shell fibers
50 by co-axial electrospinning. Polyurethane (PU) is used as core to enhance the mechanical properties
51 of the fibers; Due to the thermodynamic incompatibility between soft and hard segments in the PU
52 main chains (Skarja and Woodhouse, 1998; Hong, Guan et al., 2010), PU possesses excellent
53 mechanical properties, including high elongation at break and mechanical strength (Jiang, Greiner et
54 al., 2013; Jiang, Duan et al., 2014). The shell of the fibers consists of CAP which is widely used in
55 pharmacy and biomedicine and is highly biocompatible (McDevitt, Woodhouse et al., 2003; Guan,
56 Fujimoto et al., 2005; Tseng, Tang et al., 2005; Shau, Tseng et al., 2006; Hashizume, Fujimoto et al.,
57 2010). Also note that co-axial electrospinning is used in the biomedical field for various purposes, such
58 as to preserve unstable biological agents and viruses (Salalha, Kuhn et al., 2006), to prevent
59 decomposition of unstable compounds (Peh, Lim et al., 2015) and to achieve sustained drug release
60 (Qi, Guo et al., 2010). Also, Ball (Ball, 2014) showed that fibers obtained by co-axial electrospinning
61 allowed the sustained release of microbicides from fibers. They could deliver the compounds over
62 multiple timescales and composite microbicide fabrics were created to provide both rapid and
63 sustained drug release from a single device.

64

65 **2. Materials and methods**

66 **2.1 Materials**

67 Rhodamine B, Polyurethane (PU, $M_w = 100,000$ g/mol), 3-(2-Beenzothiazolyl)-7-(diethylamino)
68 (Coumarin 6), Tetrahydrofuran (THF), 2-Methoxyethanol, Dimethylformamide (DMF) and Acetone
69 were purchased from Daguangming (Nanjing, China). Cellulose acetate phthalate (CAP, $M_w = 60,000$

70 g/mol) was purchased from Sigma-Aldrich (Steinheim, Germany). MTT kits were purchased from
71 Aladdin (Shanghai, China). L929 cells were purchased from BioCambridge (Nanjing, China).

72

73 **2.2 Electrospun PU and CAP fibers**

74 PU (core)/CAP (shell) fibers were obtained by coaxial electrospinning a CAP solution (25%, w/v)
75 using 2-Methoxyethanol/acetone/distilled water (1:0.85:0.15, v/v/v) as solvent (Olaru and Olaru, 2010)
76 and a PU solution (14%, w/v) using a THF/DMF (1:1, v/v) as solvent. Rhodamine B was added to the
77 PU solution prior to electrospinning. PU and CAP solutions were filled in two individual syringes and
78 electrospun by one coaxial electrospinning needle with a flow rate of 0.5 ml/h for PU and 3 ml/h for
79 CAP. The fibers were collected on a metal plate. The distance between the syringe needle and the metal
80 plate was 12 cm. As a control, pure CAP and PU electrospun fiber mats were also prepared using the
81 (same) conditions as used for coaxial electrospinning. All fiber mats were vacuum dried during 24h at
82 40 °C.

83

84 **2.3 Cell culture**

85 L929 cells were maintained in 10% fetal bovine serum (FBS) supplemented Dulbecco's modified
86 Eagle's medium (DMEM, Nanjing, China) and cultured in a humid atmosphere at 37 °C with addition
87 of 5% CO₂. When the confluence reached 80% the cells were passaged. Cells were feed with fresh
88 medium three times a week.

89

90 **2.4 Cytotoxic activity**

91 To test the viability of cells exposed to electrospun fiber mats, cells were seeded in 96-well plates

92 (6000 cells/well). We used DMEM medium to make extracts from the fiber mats (1 mL DMEM was
93 used to extract 0.5 cm² fiber mats). The fiber mats were submerged into DMEM at 37 °C for 72 h.
94 After centrifugation, the supernatant ('extract') was filtered (using 0.22 μm filters); subsequently the
95 extracts were diluted in PBS. The cells were treated with (diluted) extracts at 37°C for 24h. After
96 incubating the cells with the extract, the extract was removed and the cells were washed twice with
97 PBS. Next, fresh medium containing 5 mg/ml of MTT reagent was added to the cells and incubated
98 for 4 h at 37°C. Following this incubation, the medium was carefully removed and the formazan
99 crystals were dissolved by incubation with 180 μl DMSO on a shaker for 10 min. Finally, the
100 absorbance was measured with a microplate reader at 570 nm. The percentage of viability of the cells
101 was then calculated by comparison with untreated cells representing 100% viability (so 'named relative
102 growth rate', RGR). The RGR was defined as: $RGR = A_e/A_p \times 100\%$ (1)
103 A_e being the absorbance measured in the experimental groups, A_p being the absorbance measured in
104 case DMEM medium was used.

105

106 **2.5 Rhodamine release study**

107 Rhodamine B loaded fibers were electrospun and air-dried; Therefore 1mg Rhodamine B was
108 dissolved in 0.78ml CAP solution used for electrospinning. We dispersed 5 mg of Rhodamine B-loaded
109 composite fiber mats in Eppendorf tubes filled with 1 ml of respectively pH 7.4 PBS (which served as
110 'simulated human semen', SHS) or pH 4.2 solution ('simulated vaginal fluid', SVF). The release of
111 Rhodamine B from the coaxial fibers was studied by measuring the fluorescence of the supernatant
112 (excitation light: 528 nm, emission light: 550 nm). Rhodamine B standard curves (in PBS and SVF);
113 (concentration range between 0.001 and 0.01 mg/ml) were used to determine the concentration of the

114 released Rhodamine B.

115

116 **2.6 Characterization of the fibers**

117 SEM images of the coaxial fibers were recorded by Field Emission SEM (JSM-7600F, Japan) operated
118 at an acceleration voltage of 15 kV. TEM images were captured with a JEM-2100 (Japan) transmission
119 electron microscope. The acceleration voltage was 100 kV. Rhodamine B and coumarin 6 were added
120 to stain respectively the PU solution (Red) and the CAP solution (Green). Fluorescent images of the
121 coaxial fibers were recorded by laser scanning confocal microscopy (LSCM, LSM710, Zeiss,
122 Germany). TGA of the electrospun fiber mats was performed in N₂ from 30 °C to 600 °C at 5 °C min⁻¹
123 using a universal V4.5A TA instrument. The tensile tests were carried out by a universal tensile tester,
124 equipped with a load cell which had a maximum load of 50 N and a resolution of 0.001 N. The samples
125 (20 mm × 6 mm) were stretched at a speed of 5 mm/min while the gauge length was set to 10 mm. The
126 average thickness of the samples was measured making use of a screw micrometer.

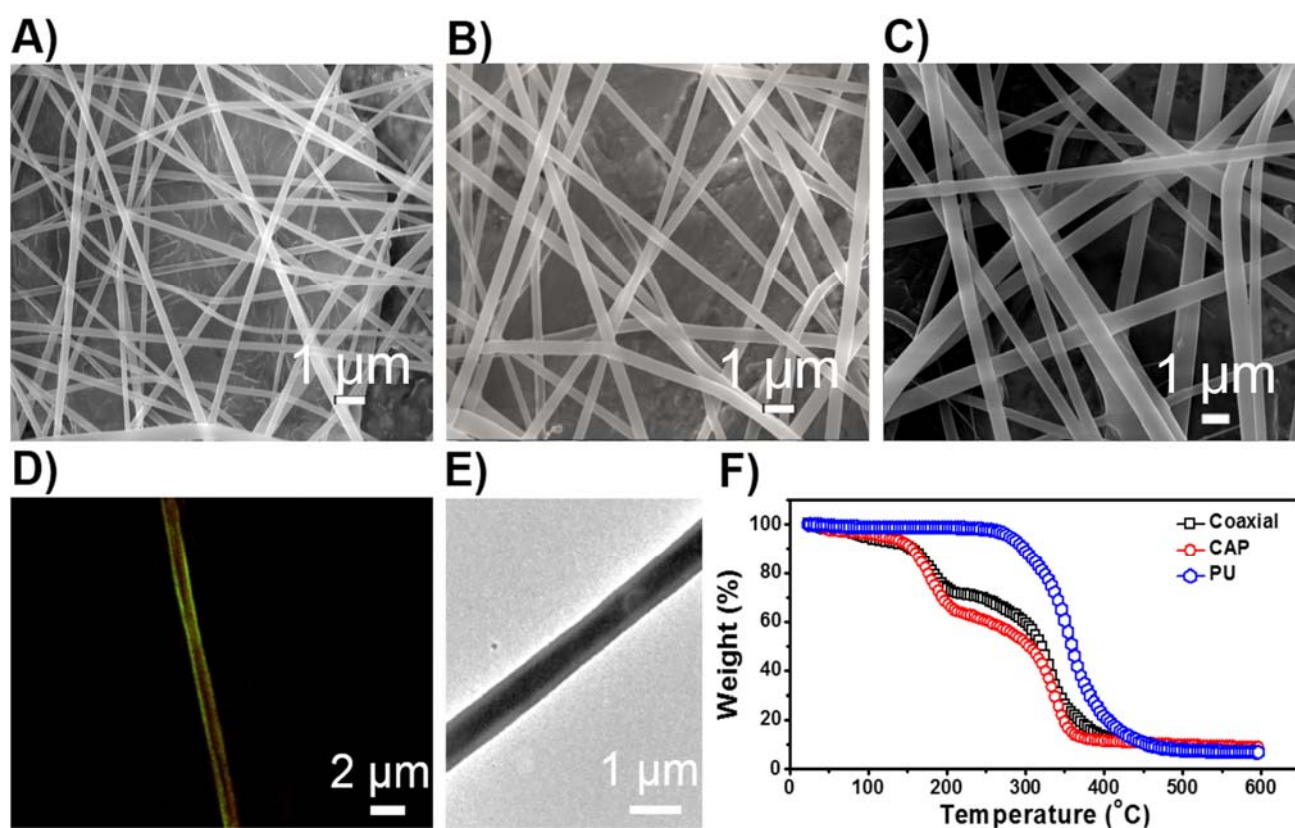
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128 **3. Results and discussion**

129 **3.1 Coaxial electrospun microfibers**

130 To overcome the poor performance of “pure” CAP electrospun fibers, coaxial electrospinning was
131 performed to incorporate PU into the core of coaxial fibers. **Figure 1A-E** shows the morphology of
132 pure CAP fibers, pure PU fibers and coaxial fibers. Both the pure CAP fibers and PU fibers possess
133 smooth surfaces (**Fig. 1A** and **1B**). The PU/CAP coaxial fiber is shown in **Fig. 1C**. The diameter of the
134 fiber was above 1 μm and the surface was smooth. The LSCM image confirmed the coaxial structure
135 of the PU/CAP fibers (**Fig. 1D**); the fiber shell was dyed green (CAP) while the fiber the core was

136 dyed red (PU). The TEM image (**Fig. 1E**) showed PU was wrapped completely in the core while there
137 was a distinct boundary between the core and shell. TGA curves of electrospun fibers are shown in
138 **Fig. 1F**. Pure PU fibers were stable until 300 °C while a three step weight loss was observed for the
139 coaxial electrospun fibers and pure CAP electrospun fibers. As the amount of PU only accounted for
140 28 wt% in the coaxial fibers, the coaxial fibers showed a similar decomposition trend as pure CAP
141 fibers, but the thermal stability was in-between pure CAP and pure PU fibers.



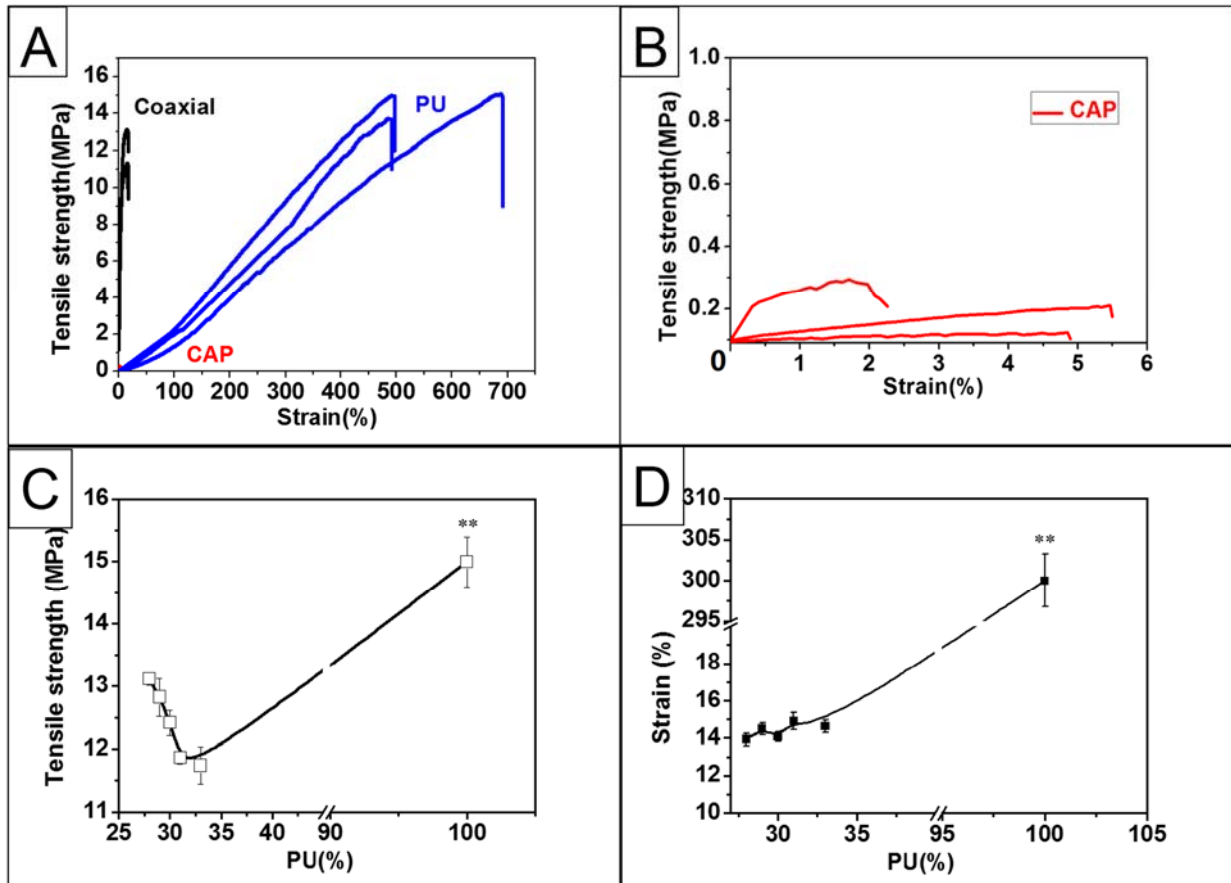
142
143 **Figure 1.** Characterization of the structure of the fibers. SEM images of A: pure CAP fibers; B: pure
144 PU fibers; C: PU/CAP coaxial fibers; D: confocal image of PU/CAP coaxial fiber (Green: CAP; Red:
145 PU); E: TEM of PU/CAP coaxial fibers; F: TGA of electrospun PU/CAP coaxial fibers (28 wt% PU),
146 pure CAP and pure PU fibers.

147

148

149 **3.2 Mechanical properties of PU/CAP coaxial microfibers**

150 Electrospun PU fibers have been reported to have excellent mechanical properties. Jiang et al. reported
151 that single electrospun PU fibers possess a tensile strength of 283 MPa and an elongation at break of
152 589 % which suggest electrospun PU fibers to be good reinforcements and toughening materials (Jiang,
153 Duan et al., 2014). However, electrospun CAP fibers showed poor mechanical properties, which limit
154 their applications. Therefore, in this work, PU was incorporated into CAP electrospun fibers by coaxial
155 electrospinning to improve the mechanical performance of CAP fibers. As shown in **Fig. 2**, pure CAP
156 and pure PU fiber mats exhibit a tensile strength of 0.2 ± 0.03 and 15.2 ± 1.18 MPa, respectively. For
157 coaxial PU/CAP fiber mats (28% PU), the tensile strength reached 13.27 ± 2.32 MPa, which is about
158 65 times that of pure CAP fibers. When the PU content increased to 33 wt%, the tensile strength
159 decreased however to 11.7 MPa. Elongation at break could be used to evaluate the flexibility of the
160 materials. Pure CAP electrospun fibers showed an elongation at break of about 4%. The incorporation
161 of PU led to significant increase in the elongation at break to about 14%, which is 250% higher than
162 that of pure CAP fibers.



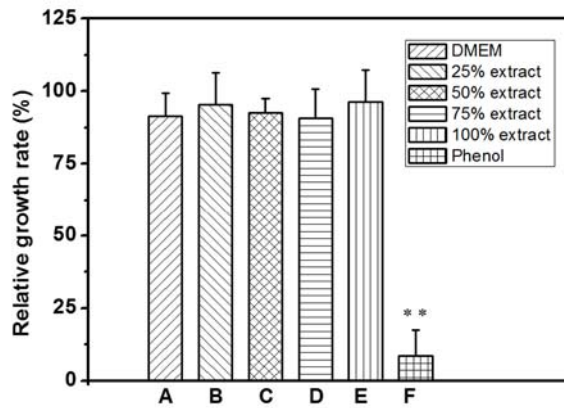
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164 **Figure 2.** (A) Tensile strength of coaxial fibers containing 28% (w/w) PU, pure PU fibers and pure
 165 CAP fibers; (B) Zoom in on the tensile strength of pure CAP fibers; (C) Tensile strength of PU/CAP
 166 coaxial fibers with different mass ratio of PU (28%, 29%, 30%, 31%, 33%, 100%); (D) Strain at break
 167 of coaxial fibers with different mass ratio of PU (28%, 29%, 30%, 31%, 33%, 100%), **significant
 168 at $p < 0.01$

169

170 3.3 Cytotoxicity assessment

171 The result of the cytotoxicity assessment is shown in **Fig. 3**. 100% (Group E) in the x-axes corresponds
 172 to the undiluted extract (see section 2.4) while 75% (v/v) (Group D), 50% (v/v) (Group C) and 25%
 173 (v/v) (Group B) refer to diluted extracts. Phenol was used as (positive) control sample (Group F).
 174 Clearly, the extracts obtained from the fibers mats did not significantly influence the cell growth.



175

176 **Figure 3.** Cytotoxicity assessment of electrospinning PU/CAP fiber mats (28wt% PU), **significant
 177 at $p < 0.01$

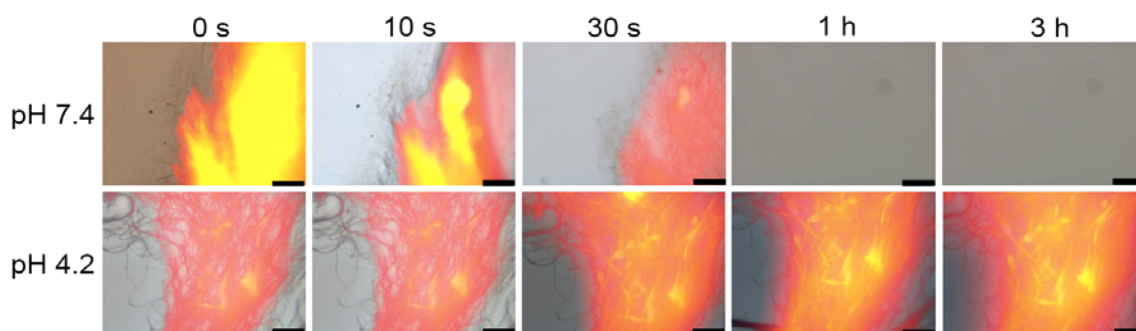
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179 3.4 Rhodamine release study

180 To investigate whether the coaxial PU/CAP fibers show pH dependent release features, fibers were
 181 exposed to pH 4.2 and pH 7.4, mimicking the pH of the simulated vaginal fluid (SVF) and semen
 182 respectively. Note that the fluorophore Rhodamine B was loaded in the CAP shell of the fibers. As can
 183 be seen from the micrographs in **Fig. 4**, at pH 4.2 the PU/CAP fiber mats remain loaded with
 184 Rhodamine B, even after 3 h. In contrast, the fluorophore was immediately released from the fibers at
 185 pH 7.4. Fluorescence measurements (**Fig. 5**) confirmed that coaxial PU/CAP fibers retained
 186 Rhodamine B at acidic (vaginal) pH while they released it rapidly (within 1 minute) at pH 7.4. In
 187 agreement, we observed by dissolution tests that the coaxial fibers were completely dissolved in pH
 188 7.4 PBS in 1 min. By electrospinning three-dimensional fiber mats with a large specific surface area
 189 are obtained which facilitates water absorption and release of the compound encapsulated from the
 190 CAP-shell into the water.

191

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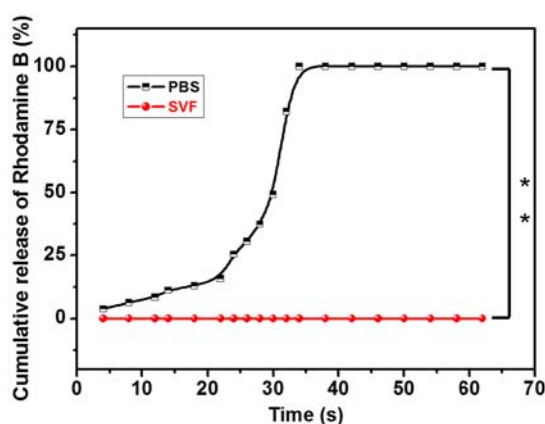


193

194 **Figure 4.** Fluorescence microscopy on Rhodamine B-loaded PU/CAP coaxial fibers (28% w/w PU)
195 dispersed in respectively SVF and PBS. Scale bar = 50 μ m.

196

197



198

199 **Figure 5.** Release profile of Rhodamine B from electrospun fibers in respectively SVF and PBS
200 (appropriate standard curves of Rhodamine B in SVF and PBS were used to calculate the concentration
201 of released Rhodamine B), **significant at $p < 0.01$

202

203 4. Conclusions

204 In this study we prepared and characterized PU/CAP coaxial fibers with improved mechanical
205 properties and investigated their potential as semen sensitive delivery system. We observed that,

206 compared to previously reported CAP fibers, the coaxial structure of PU/CAP fibers significantly
207 improved the mechanical strength of the fibers. Our data show that the coaxial fibers remain intact in
208 SVF at pH 4.2 while they dissolve very rapidly in PBS at pH 7.4. Extracts obtained from the fiber
209 mats did not induce cytotoxicity. The core-shell PU/CAP coaxial fibers showed an outspoken pH
210 responsive release of Rhodamine which allows us to conclude that PU/CAP coaxial electrospun fibers
211 mats are promising for pH responsive drug delivery, especially in the context of semen sensitive drug
212 release.

213

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