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#### ▶ To cite this version:

Jérôme Fehrenbach, Lisl Weynans. Activation Sites Estimation using a Fast Algorithm Based on an Eikonal Equation. Computing in Cardiology: CINC 2022, Sep 2022, Tampere, Finland. hal-03913733

#### HAL Id: hal-03913733 https://hal.inria.fr/hal-03913733

Submitted on 27 Dec 2022

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# **Activation Sites Estimation using a Fast Algorithm Based on an Eikonal Equation**

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### **Context and objectives**

- Classical algorithms for ECGI solve at each time instant an static and extremely ill-posed inverse problem, requiring an adequate regularization strategy (or instance Tikhonov)
- An alternative way of regularizing the inverse problem is to consider information from other time steps, taking into account that electric potentials in the heart are obtained by the propagation of an electric wave.
- Our objectives: design a fast algorithm based on a simple activation front model to retrieve significant features of the ECGI

#### Test case: Localization of 2 sources and metric estimation



Figure: Left: evolution of the cost function J. Right: evolution of the distance to the solution  $||x^k - x^*||$ .



### inverse problem

### **Propagation model**

- We consider in the present work only the surface of the heart
- Anisotropic eikonal equation: simplified model of electrical activation front in asymptotic regime:

$$\left\{ egin{array}{l} \| 
abla T \|_{D(x)}^2 = 1, \ T(x_i^0) = au_i, i = 1 \dots s, \end{array} 
ight.$$

#### with

- $\triangleright$  T depolarization time of heart surface,
- $\triangleright$  D(x) tensor quantity describing the anisotropic conduction  $\succ$   $\tau_i$  activation times at sources  $x_i^0$  (earliest activation sites)
- $\Rightarrow$  parameters elevant in the context of EGCI
- T(x) is also the length of the shortest path joining the sources to x





Figure: Left: location of the successive iterates  $x^k$  (red) and the true source point  $x^*$ (blue). Right: evolution of the parameters of the metric.

# Test case: mimicking an ECG inversion





Figure: Example of solution of eikonal equation with anisotropic conduction

## Methods

- Iterative algorithm to minimize misfit between observations and predictions of the model
- Cost function

 $J(\mathbf{x},\tau) = \frac{1}{2} \|G(\tau + \phi_{\mathbf{x}}) - g^{\text{OBS}}\|_{Y}^{2}.$ 

with G observation operator (on heart or torso surface), x sources location,  $g^{OBS}$  observations with noise

- Least square minimization with Gauss Newton algorithm
- Sensitivity of cost function with respect to source locations and activation times depends on **Logarithmic map**:

if  $\gamma$  is a unique shortest geodesic path from point x to point y then  $Log_x(y) = \gamma'(0) =$  initial direction of  $\gamma$ 

Figure: Left: configuration of the torso (electrodes in red) and the heart surface (visible by transparency). Right: location of the successive iterates  $x^k$  (red) and the true source point *x*<sup>\*</sup> (blue)



Figure: Left: evolution of the cost function J. Right: evolution of the distance to the solution  $||x^k - x^*||$ .

#### Conclusion

- Efficient new method to estimate sources and activation times in the eikonal equation on a surface  $\Rightarrow$  applicable to ECGI.
- In case of complex or pathological propagation patterns, need to extend the method to a cardiac volume.

# Vector Heat Method: efficient computational method to compute Logarithmic map, avoiding to compute all geodesics



#### Figure: Illustration of Log map from et al

#### References

[1] J. Fehrenbach, L. Weynans, Source and metric estimation in the eikonal equation using optimization on a manifold, under revision [2] Grandits et al, GEASI: Geodesic-based Earliest Activation Sites Identification in cardiac models, Int. J. Numer. Meth. Biomed *Engng*, 2021 [3] N. Sharp et al, The vector heat method. ACM Transactions on Graphics, 2019.







